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(54) **REUSABLE MR SAFE TEMPERATURE
PROBE FOR SURFACE AND BODY
TEMPERATURE MEASUREMENT**

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See application file for complete search history.

(56) **References Cited**

U.S. PATENT DOCUMENTS

3,190,436 A 6/1965 Diamant
3,315,797 A 4/1967 Olsson
(Continued)

FOREIGN PATENT DOCUMENTS

EP 0336984 A1 * 10/1989 A61B 5/14539
WO 0223148 A1 3/2002
WO 2010102117 A1 9/2010

OTHER PUBLICATIONS

Somnex, "MRI active guidewire with an embedded temperature
probe and providing a distinct tip signal to enhance clinical safety",
Journal of Cardiovascular Magnetic Resonance 12:38, 2012 (Year:
2012).*

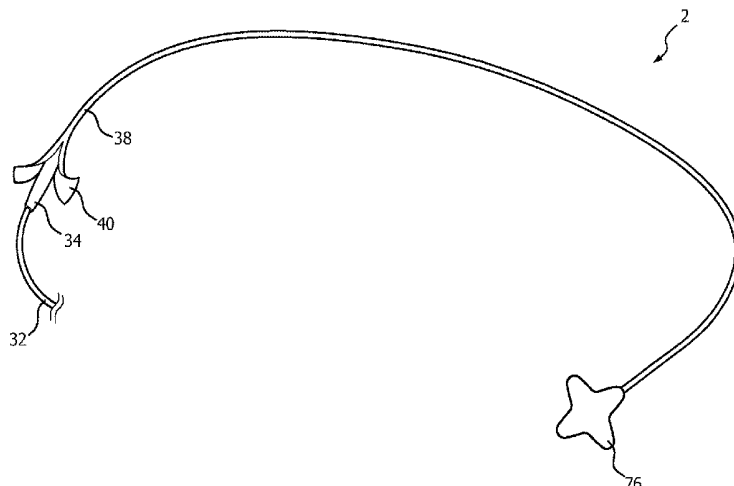
(Continued)

Primary Examiner — Joanne M Hoffman

(57) **ABSTRACT**

A magnetic resonance probe (2) includes a fiber optic sensor
probe (32) and a sheath (38). The fiber optic sensor probe
(32) includes a non-ferrous sensor (42) on a distal portion
(36) configured for insertion into a subject, a locking ele-
ment (34) connected to the distal portion (36), and a proxi-
mal portion (44) connected to the locking element (34) and
in light communication via an optical fiber (48) with the

(Continued)



non-ferrous sensor (42) and includes a connector (46). The sheath (38) covers the distal portion (36) of the fiber optic sensor probe (32), engages the locking element (34), and provides a sterile outer surface (70).

14 Claims, 9 Drawing Sheets

(56)

References Cited

U.S. PATENT DOCUMENTS

3,552,558 A * 1/1971 Poncy G01K 1/083
206/306
3,732,975 A * 5/1973 Poncy G01K 1/083
206/212
3,752,309 A * 8/1973 Hopkins G01K 1/083
206/306
3,822,593 A 7/1974 Oudewaal
4,026,751 A * 5/1977 Fowler G01K 1/08
156/290
D252,104 S 6/1979 Nagy et al.
4,165,000 A * 8/1979 Poncy G01K 1/083
206/306
4,306,562 A * 12/1981 Osborne A61M 25/0668
604/164.05
4,392,005 A * 7/1983 Mohrman G01K 13/002
136/221
4,402,685 A * 9/1983 Buhler A61L 29/049
525/931
4,449,973 A * 5/1984 Luther A61M 25/065
604/161
4,596,559 A * 6/1986 Fleischhacker ... A61M 25/0668
604/161
D300,609 S 4/1989 Leverty
4,911,559 A 3/1990 Meyst et al.
4,983,168 A * 1/1991 Moorehead A61M 25/0668
604/161
RE33,854 E * 3/1992 Adair A61B 1/00101
600/109
5,167,634 A * 12/1992 Corrigan, Jr. A61M 25/0668
604/160
5,221,263 A * 6/1993 Sinko A61M 25/0668
604/161
5,273,041 A * 12/1993 Richards A61B 5/055
600/411
5,280,173 A 1/1994 Morse et al.
5,383,453 A * 1/1995 Fischer A61B 5/14539
29/428
5,588,432 A * 12/1996 Crowley A61B 5/02007
600/374
5,713,867 A * 2/1998 Morris A61M 25/0668
604/164.05
5,738,632 A * 4/1998 Karasawa G01R 33/285
324/318
5,771,327 A * 6/1998 Bar-Or G02B 6/3849
385/139
5,930,440 A * 7/1999 Bar-Or G02B 6/241
385/136
5,997,562 A * 12/1999 Zadno-Azizi A61M 25/0662
604/158
6,216,030 B1 * 4/2001 Howard A61M 25/0105
600/427
6,358,460 B1 * 3/2002 Hunt, Jr. B29D 23/001
264/491
6,454,744 B1 * 9/2002 Spohn A61M 25/0668
604/164.05
6,463,187 B1 * 10/2002 Baruch A61B 5/021
385/12
6,574,497 B1 6/2003 Pacetti
6,716,223 B2 * 4/2004 Leopold A61M 25/0668
606/144
6,738,145 B2 5/2004 Sherrer et al.
7,011,647 B2 3/2006 Purdy et al.

7,048,732 B2 5/2006 Ellingsen
7,160,291 B2 * 1/2007 Damasco A61B 18/02
606/20
7,187,964 B2 * 3/2007 Khoury A61B 5/0422
600/509
7,684,657 B2 3/2010 Donlagic et al.
7,720,532 B2 * 5/2010 Hashimshony A61B 34/20
600/439
7,762,995 B2 7/2010 Eversull et al.
9,360,643 B2 * 6/2016 Rinzler G02B 6/3813
2001/0038453 A1 * 11/2001 Jung G01J 3/02
356/419
2002/0022832 A1 2/2002 Mikus et al.
2002/0029054 A1 * 3/2002 Rabiner A61B 17/320068
606/169
2002/0147394 A1 * 10/2002 Ellingsen A61B 5/01
600/410
2002/0159671 A1 10/2002 Boyd et al.
2004/0122494 A1 * 6/2004 Eggers A61B 18/04
607/103
2004/0186377 A1 9/2004 Zhong et al.
2004/0236314 A1 * 11/2004 Saab A61M 39/0247
604/539
2005/0177025 A1 * 8/2005 Jaker A61B 1/00135
600/121
2005/0194979 A1 * 9/2005 Roman G01R 31/1272
324/536
2005/0195402 A1 9/2005 May et al.
2005/0215874 A1 9/2005 Wang et al.
2005/0231729 A1 10/2005 Lopushansky et al.
2006/0115202 A1 6/2006 Stevens et al.
2008/0097193 A1 * 4/2008 Karmarkar A61B 5/055
600/423
2009/0012511 A1 * 1/2009 Welches A61B 18/201
606/15
2009/0171238 A1 * 7/2009 Hanley A61B 5/01
600/549
2009/0306591 A1 * 12/2009 Amisar A61M 25/01
604/122
2010/0066371 A1 * 3/2010 Vij A61B 5/055
324/318
2011/0301508 A1 * 12/2011 Sethuraman A61N 7/022
601/2
2012/0039357 A1 2/2012 Levesque et al.
2012/0184842 A1 * 7/2012 Boularot A61B 5/0068
600/411
2013/0197498 A1 * 8/2013 Laske A61B 18/02
606/21
2014/0012155 A1 * 1/2014 Flaherty A61B 5/015
600/549
2014/0128881 A1 * 5/2014 Tyc A61B 18/22
606/130
2015/0289929 A1 * 10/2015 Toth A61B 18/1492
600/372
2015/0297246 A1 * 10/2015 Patel A61B 17/1671
606/79
2017/0143214 A1 * 5/2017 Garibotto A61B 5/6852

OTHER PUBLICATIONS

Biopac Systems Inc.; Phychophysiology: Fiber Optic Temperature Rectal Probe; product description <http://www.biopac.com/Research.asp?Pid=4892> accessed Aug. 17, 2012.
Budelmann, C., et al.; Electronic Sensor Nodes Powered over Fibre Optimized for Ultra-Precise Temperature Measurements in Magneticresonance Imaging Machines; 2012; 1st Joint International Symposium on System Integrated Intelligence; vol. 1; pp. 189-191.
De Jonckheere, J., et al.; OFSETH: Optical Fibre Embedded into technical Textile for Healthcare, an efficient way to monitor patient under magnetic resonance imaging; 2007; IEEE EMBS; pp. 3950-3953.
Nasr, V. G., et al.; Performance Validation of a Modified Magnetic Resonance Imaging-Compatible Temperature Probe in Children; 2012; Anesthesia & Analgesia; 114(6)1230-1234.
Park, Y-L., et al.; MRI-compatible Haptics: Strain sensing for

(56)

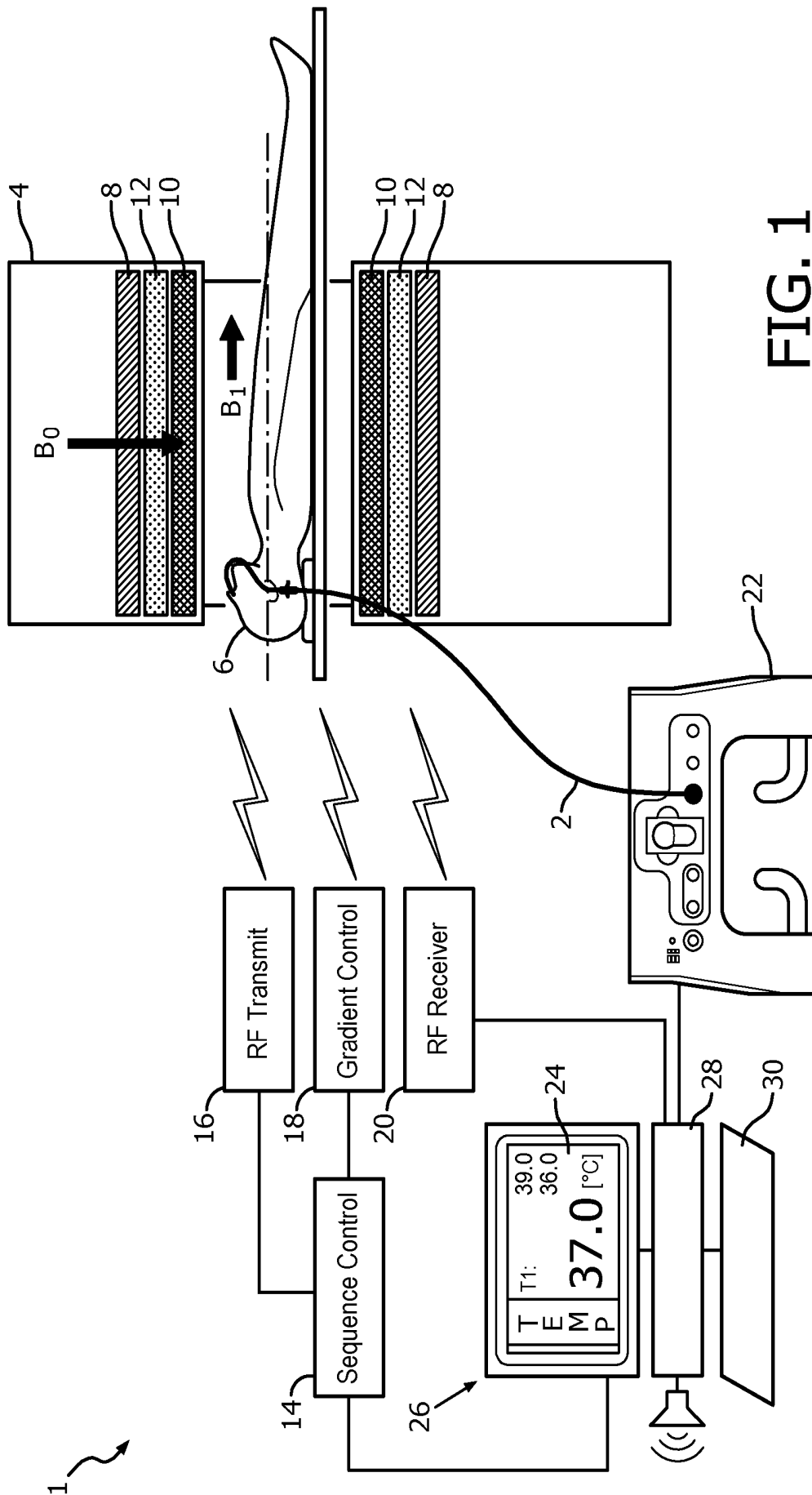
References Cited

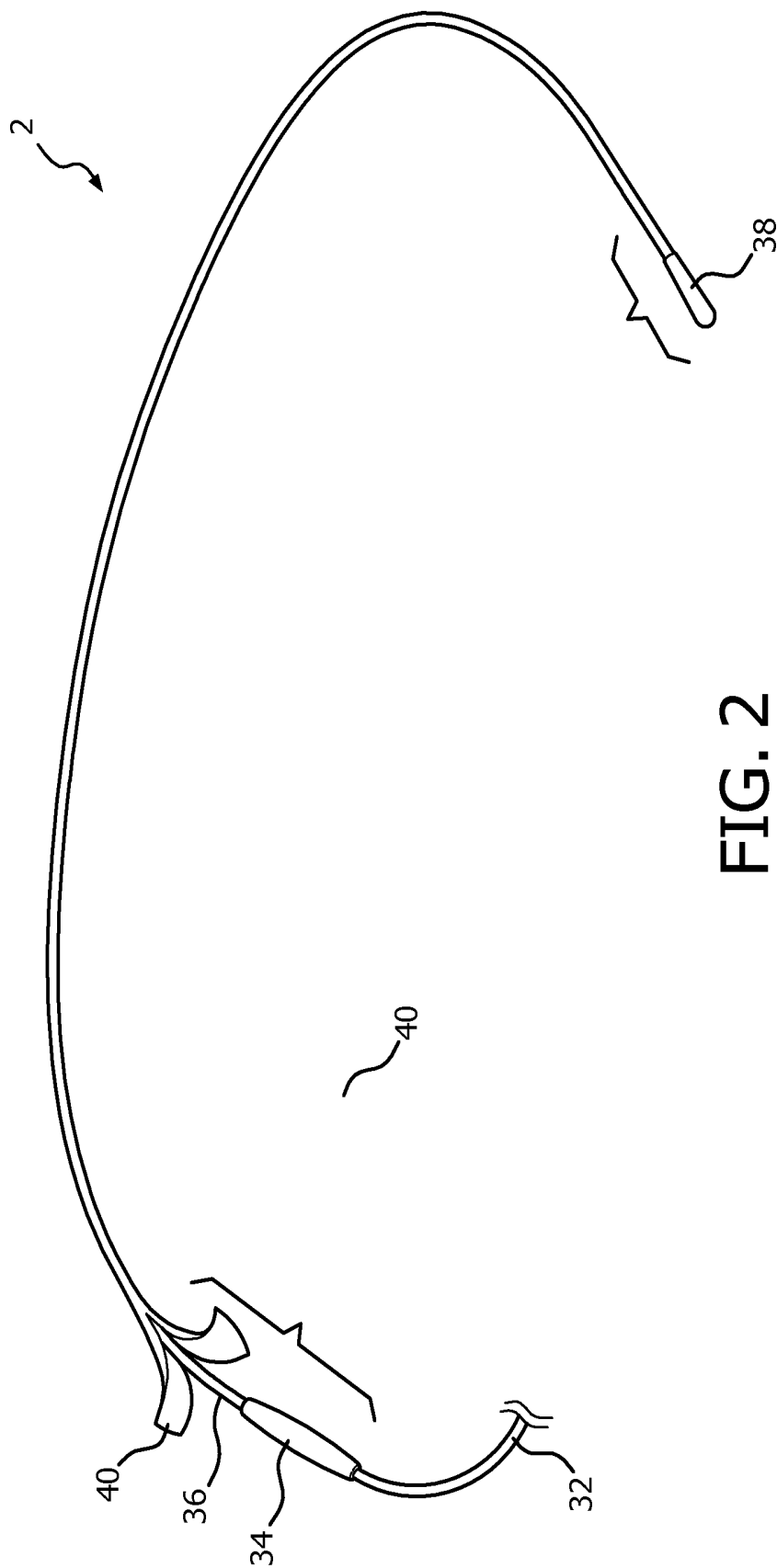
OTHER PUBLICATIONS

real-time estimation of three dimensional needle deflection in MRI environments; 2009; Int'l. Proc. MRM; vol. 17:63.

Sonmez, M., et al.; MRI active guidewire with an embedded temperature probe and providing a distinct tip signal to enhance clinical safety; 2012; Journal of Cardiovascular Magnetic Resonance; 14:38.

* cited by examiner





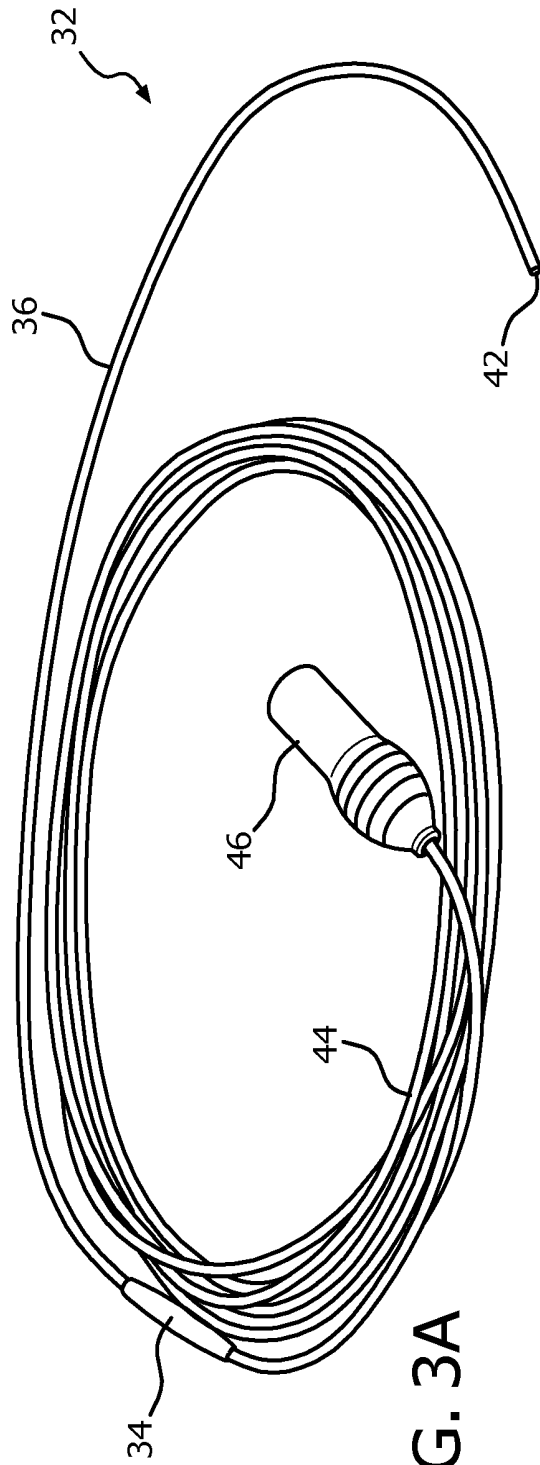


FIG. 3A

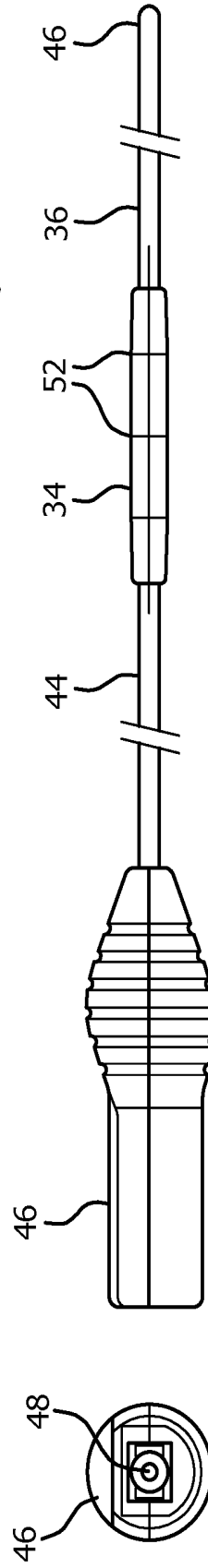


FIG. 3B

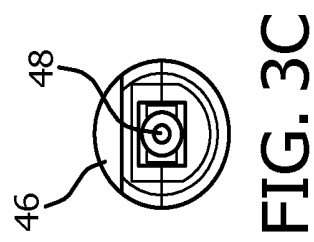


FIG. 3C

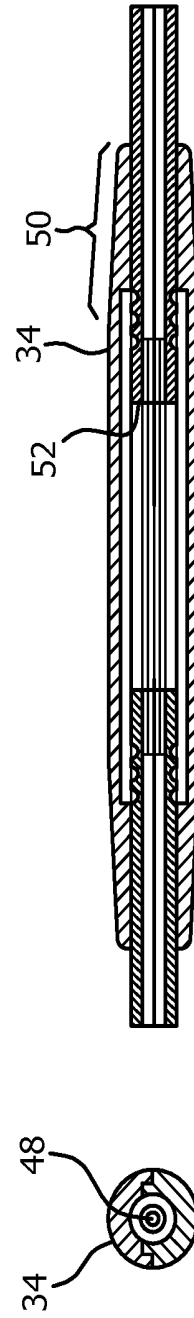


FIG. 3D

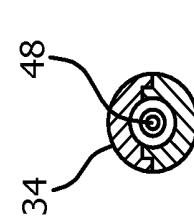
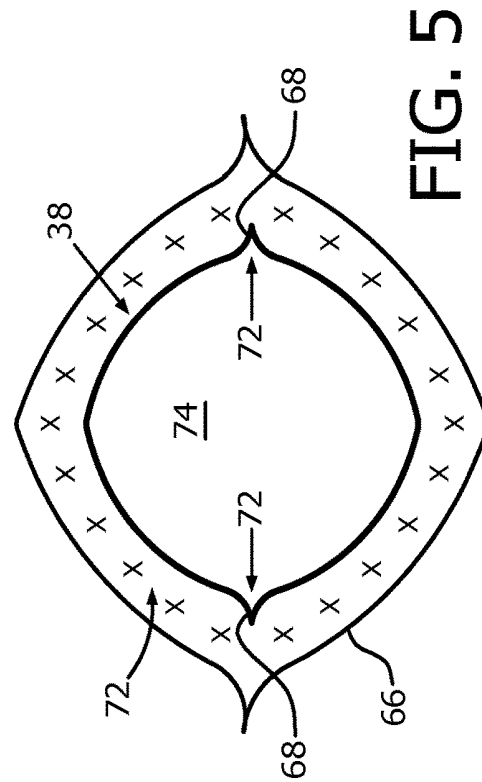
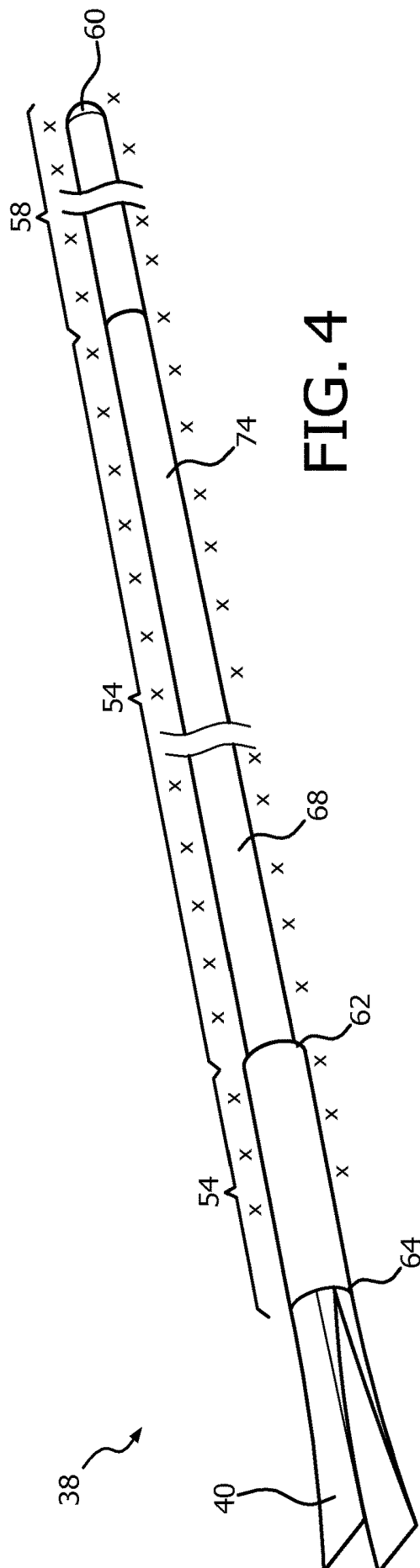


FIG. 3E



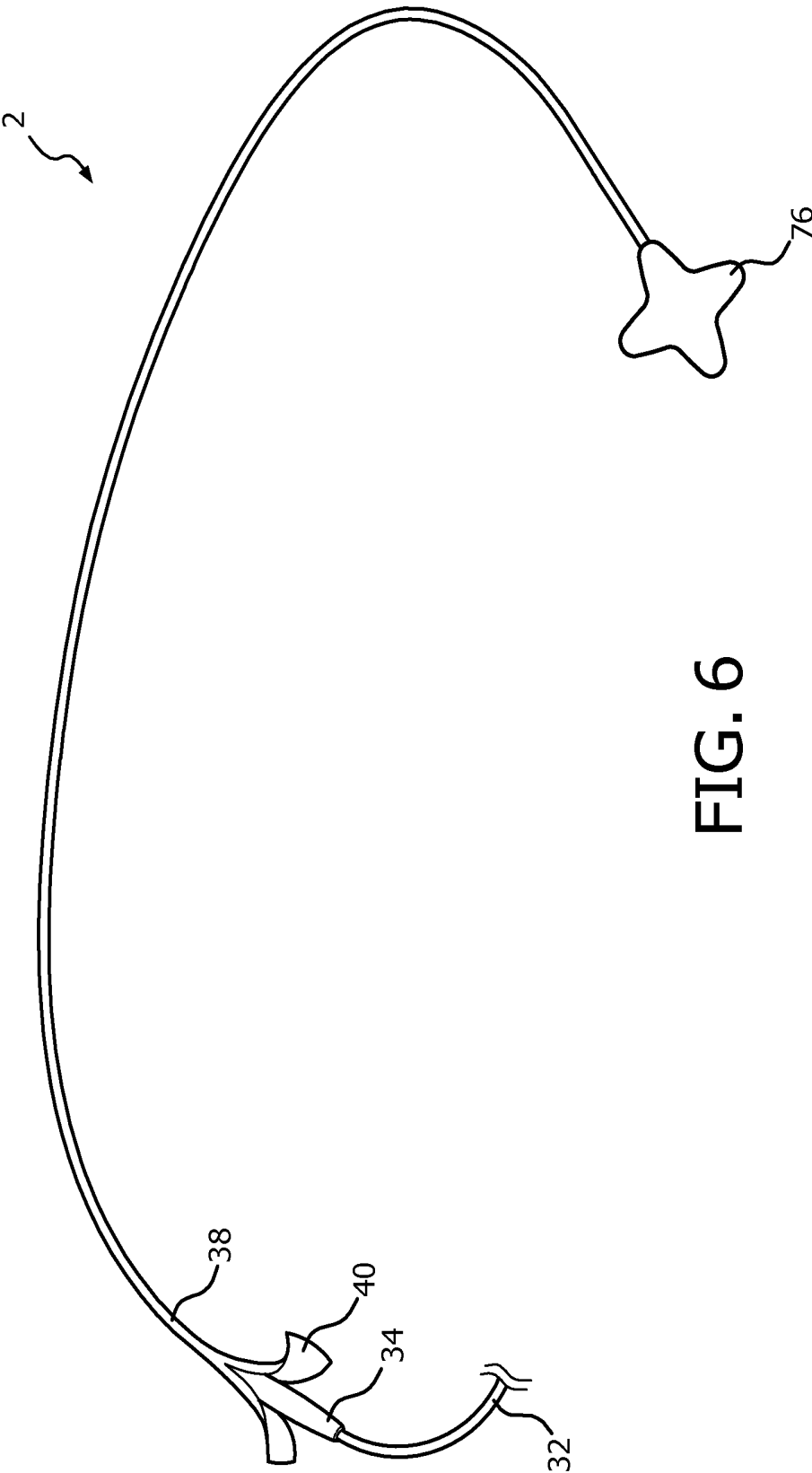
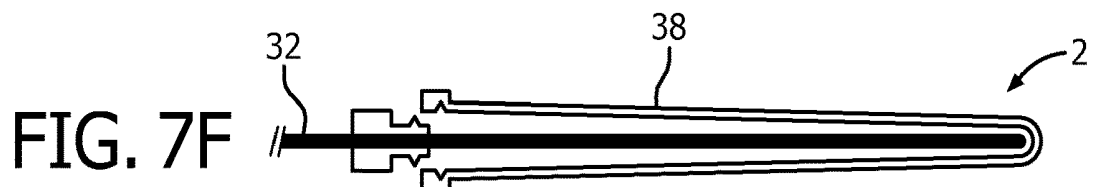
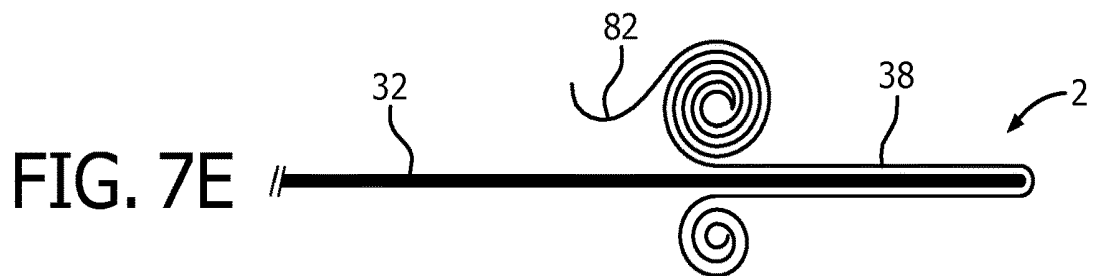
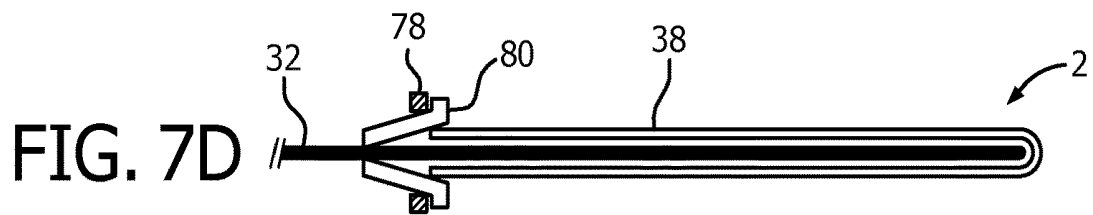
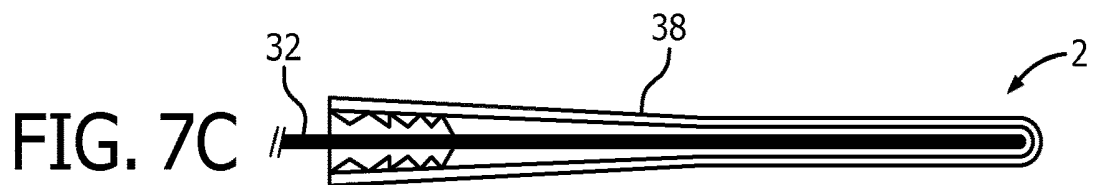
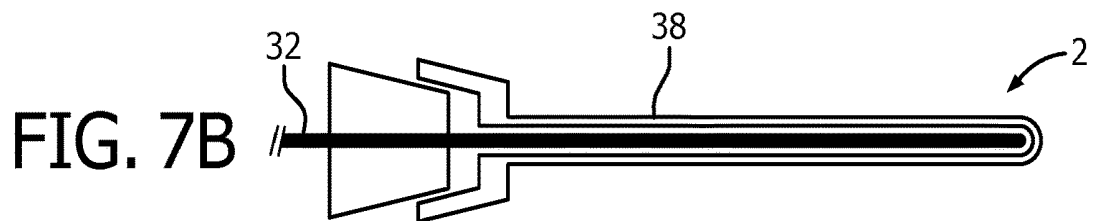
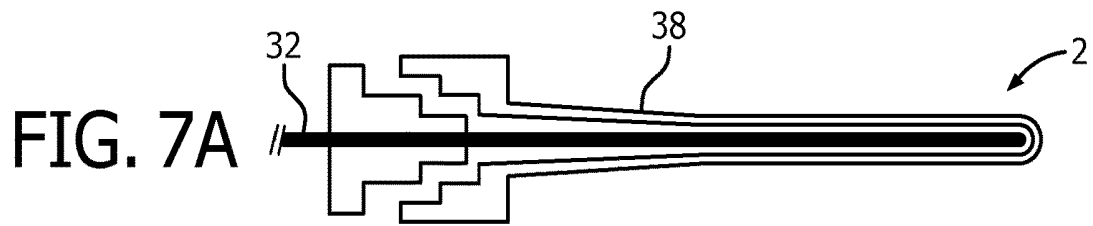
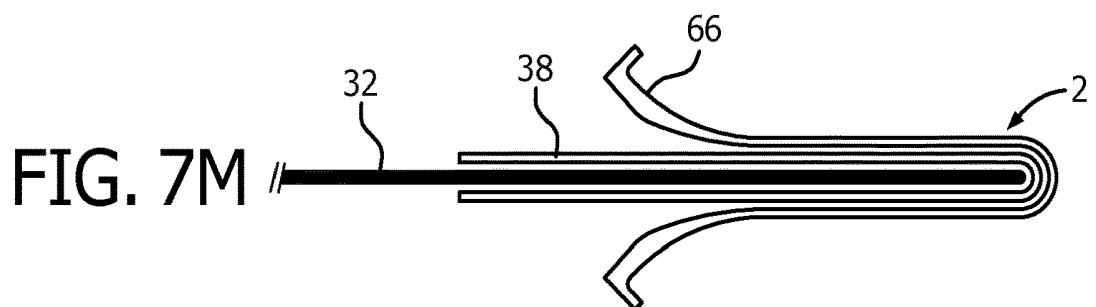
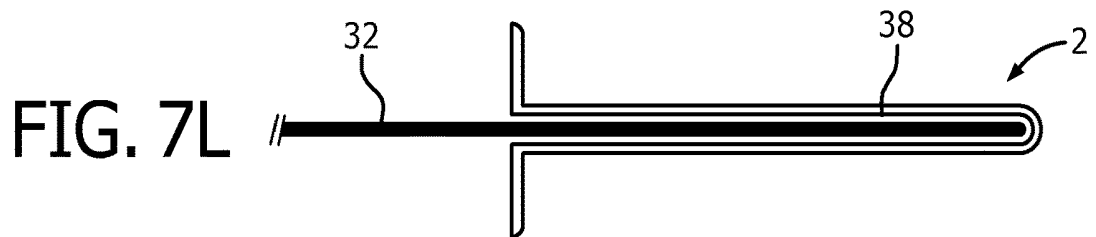
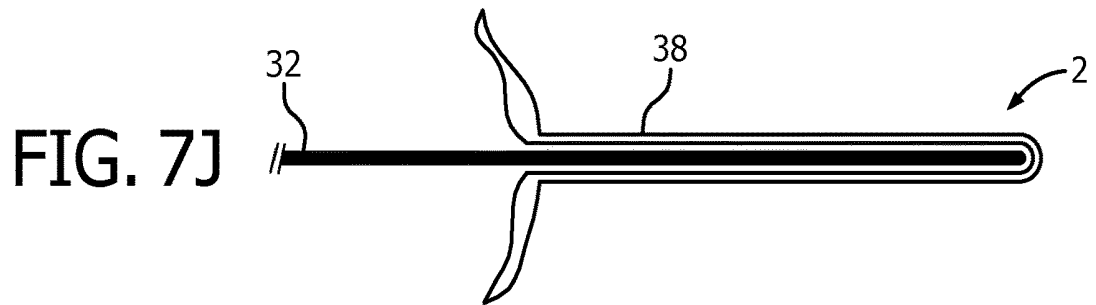
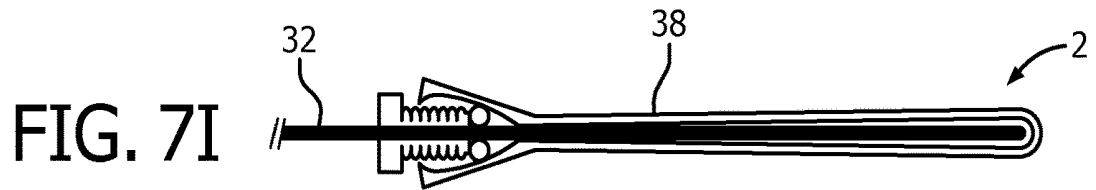
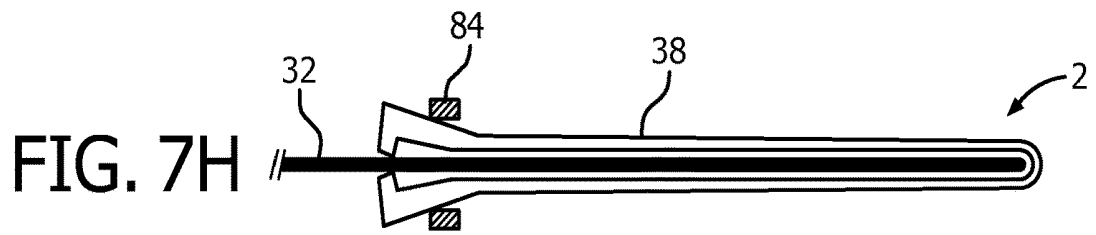
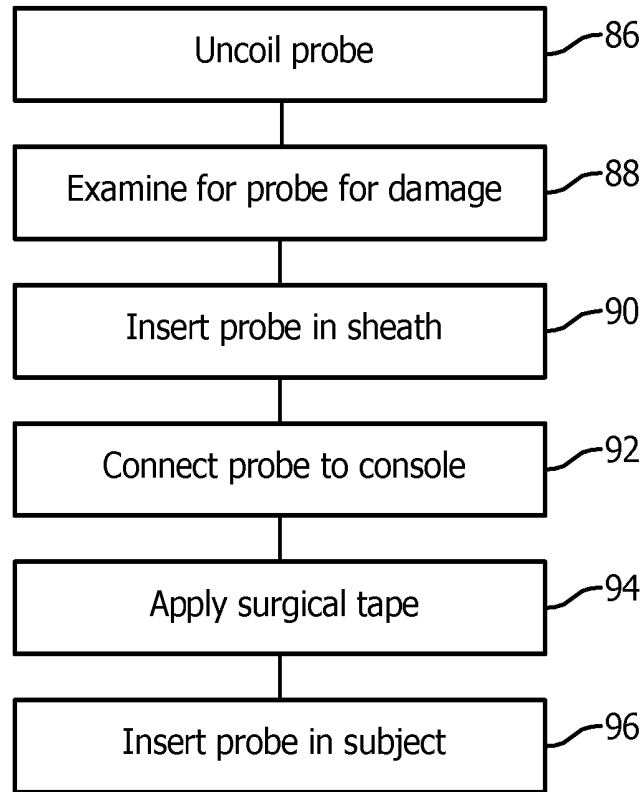
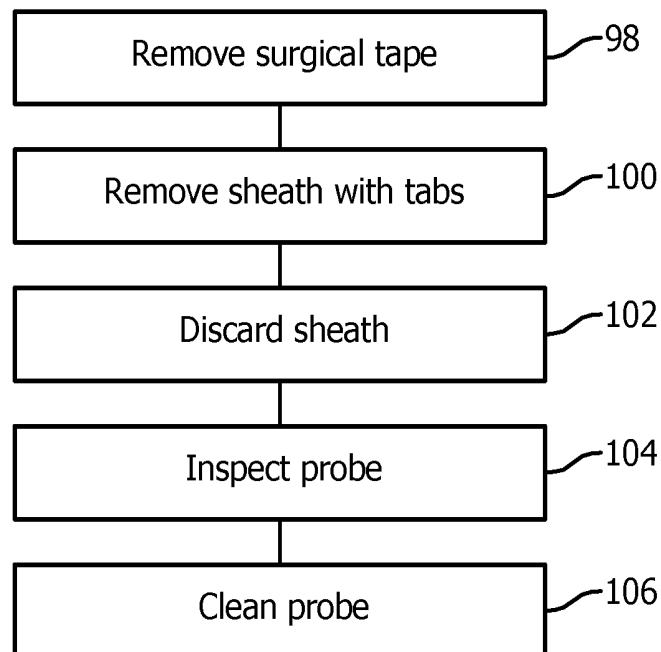
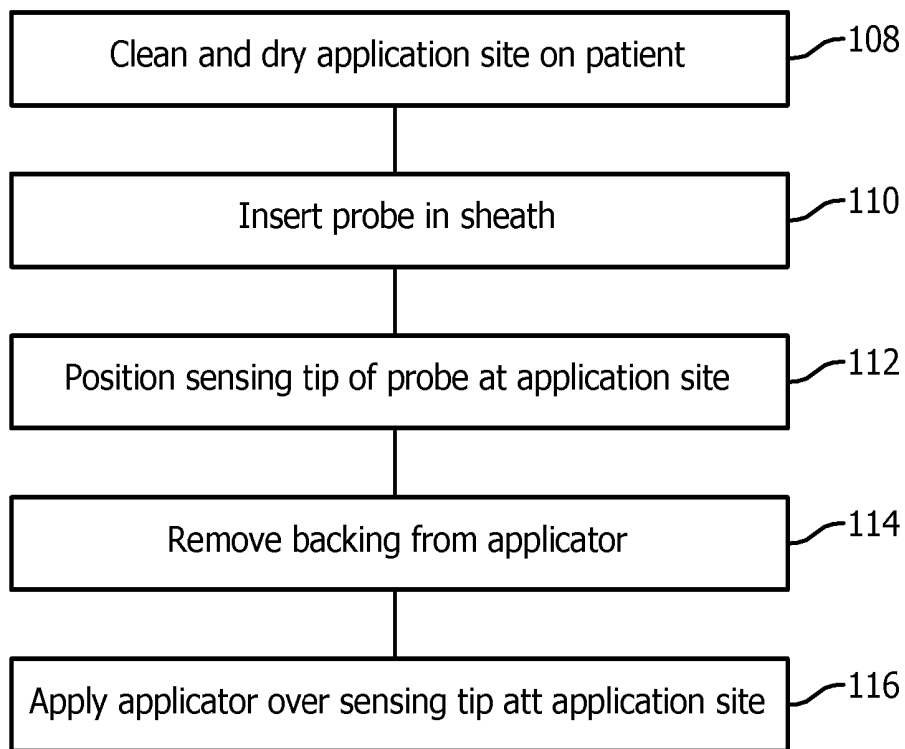


FIG. 6





**FIG. 8****FIG. 9**

**FIG. 10**

REUSABLE MR SAFE TEMPERATURE PROBE FOR SURFACE AND BODY TEMPERATURE MEASUREMENT

CROSS REFERENCE TO RELATED APPLICATIONS

This application is a national filing of PCT application Serial No. PCT/IB2013/060765, filed Dec. 10, 2013, published as WO 2014/097049 A2 on Jun. 26, 2014, which claims the benefit of U.S. provisional application Ser. No. 61/738,460 filed Dec. 18, 2012, which is incorporated herein by reference.

The following relates generally to magnetic resonance imaging and temperature sensing. It finds particular application in conjunction with non-ferrous sterile temperature sensing, and will be described with particular reference thereto. However, it will be understood that it also finds application in other usage scenarios and is not necessarily limited to the aforementioned application.

During magnetic resonance (MR) imaging, patient vital signs are frequently monitored such as the temperature of a patient. Monitoring can include a surface temperature with a probe placed against the skin of the patient or internally in the gut such as through the esophagus or the rectum. Temperature can also be used as part of an imaging protocol where temperature can affect quantitative measurement such as diffusion rates in angiograms.

Safe temperature probes in magnetic resonance imaging ideally use non-conductive, non-ferrous materials. Magnetic resonance uses strong radio frequency (RF) and gradient magnetic fields which can induce currents in conductive materials. Ferrous materials can cause aberrations in magnetic fields. Conductive materials with induced currents can cause unsafe conditions for the patient such as the potential for patient burns.

The material used during magnetic resonance imaging should not affect the imaging. That is, the material should be invisible to the magnetic resonance imaging and not emit proton resonance. Improper selection of materials can cause distortions or gaps in the MR signals which cause distortions or gaps in the MR images.

The protocols and procedures used before, during, and after magnetic resonance imaging vary and accommodate a wide variety of situations that call for flexibility of the temperature probe. For example, a surface temperature may be all that is called for by one situation, while a different patient protocol may call for an internal temperature. In order to provide an efficient and effective workflow, the workflow and tools used for MR imaging should accommodate the variety of situations with minimal change in tools such as the temperature probe. The time to measure the temperature is called the response time and includes the time from the application of the probe to the body surface or internally to the time of temperature measurement. The response time is based on the material properties including thickness used to measure the temperature. The response time affects the clinical workflow. Too long a response time is undesirable in measuring patient vital signs and/or measuring changes for a clinical protocol and may pose a risk to the patient.

For internal usage, the probe is sterile and biocompatible. Typically, MR probes used internally are disposable because of the difficulty of sterilization for reuse. For example, a fiber optic probe such as a single piece Fabry-Perot optical sensor can be used in MR imaging, but the materials in the probe are not easily sterilized. Heat is one method of

sterilization which is not compatible with fiber optics. Alternatively, chemicals and/or abrasives can be used, but can also damage the fiber optics. Typically, fiber optic temperature probes, although expensive, are used as disposable probes.

Probe materials of an internal probe are often bent to pass through the nasal passage into the esophagus. The probe needs to accommodate the size and bending within the small nasal passage during insertion and removal. A stiff probe can damage the cavity and harm the patient. The probe during insertion and removal should be strong enough not to break or leave components in the patient. The sterile portion of a probe which is inserted into the patient can be as long as 50 cm.

The following discloses a new and improved reusable MR safe probe which addresses the above referenced issues, and others.

In accordance with one aspect, a magnetic resonance probe includes a fiber optic sensor probe and a sheath. The fiber optic sensor probe includes a non-ferrous sensor on a distal portion configured for insertion into a subject, a locking element connected to the distal portion, and a proximal portion connected to the locking element and in light communication via an optical fiber with the non-ferrous sensor and includes a connector. The sheath covers the distal portion of the fiber optic sensor probe, engages the locking element, and provides a sterile outer surface.

In accordance with another aspect, a sterile sheath includes a tube of a material which produces no magnetic resonance signal and configured with a cavity open at one end and to receive and enclose at least one non-ferrous sensor located at an end of a fiber optic sensor probe, closed at an other end, and which provides a sterile outer surface.

In accordance with another aspect, a method for configuring a magnetic resonance temperature probe includes inserting a non-ferrous temperature sensor on a distal portion of a fiber optic sensor probe into a sterile sheath which produces no magnetic resonance signal and covers the distal portion of the fiber optic sensor probe, and the proximal end of the sheath frictionally engages a locking element connected to the distal portion of the probe.

One advantage is a sterile temperature probe which is MR safe and reusable.

Another advantage resides in accommodating surface and internal uses with a single probe.

Another advantage resides in the material size, flexibility, and strength for internal usage.

Another advantage resides in ease of use in an MR clinical workflow.

Another advantage resides in the disposable sterile sheath.

Another advantage resides in the coupling of the disposable sterile sheath and the fiber optic temperature probe.

Still further advantages will be appreciated to those of ordinary skill in the art upon reading and understanding the following detailed description.

The invention may take form in various components and arrangements of components, and in various steps and arrangement of steps. The drawings are only for purposes of illustrating the preferred embodiments and are not to be construed as limiting the invention.

FIG. 1 schematically illustrates an embodiment of a magnetic resonance system with a reusable MR safe probe.

FIG. 2 schematically illustrates one embodiment of a reusable MR safe probe.

FIGS. 3A-3E schematically illustrate an embodiment of a fiber optic sensor probe.

FIG. 4 illustrates an embodiment of a sheath in perspective.

FIG. 5 illustrates an embodiment of a sheath with a cover in a cross section view.

FIG. 6 illustrates an embodiment of the reusable MR safe probe with a surface application.

FIGS. 7A-7M diagrammatically illustrate various embodiments of the reusable MR safe probe and sheath.

FIG. 8 flowcharts one method of configuring the reusable MR safe probe for insertion into a subject.

FIG. 9 flowcharts one method of removing the sheath from the reusable MR safe probe.

FIG. 10 flowcharts one method of configuring the reusable MR safe probe for a surface application.

With reference to FIG. 1, an embodiment of a magnetic resonance system 1 with a reusable MR safe probe 2 is schematically illustrated. The system 1 includes a MR scanner 4 such as an open system or c-type scanner, a horizontal bore scanner, and the like shown in a cross section view. The scanner includes an opening or bore that defines an examination region in which a subject 6 is placed for a spectroscopic and/or imaging examination. The MR scanner 4 includes one or more main magnets 8 with a C-shape ferrous flux return path, one or more radio frequency (RF) coils 10, and one or more gradient coils 12.

The system 1 includes a sequence controller 14 which controls the operation of the imaging sequence, a RF transmitter unit 16 controlling the operation of the RF coils 10, and a gradient controller 18 controlling the operation of the gradient coils 12. The communication between the controlling unit and the corresponding coils can be wireless or wired. The RF coils 10 generate radio frequency pulses which excite and manipulate resonance in tissue of the subject 6. The RF coils 10 can include a whole body coil and/or a local coil such as a torso coil, hand coil, shoulder coil, knee coil, etc. The one or more gradient coils 12 generate gradient magnetic fields across the static magnetic field to spatially encode the induced resonance, induced gradient echoes, and the like. The sequence controller 14 configures the RF coils and the gradient coils to excite and manipulate resonance in tissues of the subject.

The system 10 includes a RF receiver unit 20, which receives MR signals. As the resonance decays in the tissue of the subject, weak radio frequency signals or MR signals are received by a radio frequency antenna such as the RF coils 10 and transmitted to the RF receiver unit 20. A reconstruction unit, such as a processor, receives RF data or MR signals from the RF receiver 20 and reconstructs one or more images from the received MR data such as image slices, a volume, etc.

The reusable MR safe probe 2 can be used during a MR imaging procedure or in the presence of the MR scanner 4 at any time. The reusable MR safe probe can be used internally by insertion into the gut of the subject 6 such as either through the nasal passage into the esophagus or the rectum. The reusable MR safe probe has flexibility and size to bend around and pass through the nasal passages of the subject. The reusable MR safe probe 2 includes material which produces no or a minimal MR signal, e.g. emits no proton resonance during excitation or in the presence of the magnetic fields generated by the main magnet coils 8 or the gradient coils 12. The portion of the probe 2 which is inserted into the subject includes an outer surface which is sterile and non-permeable, and includes at least one non-ferrous sensor such as a temperature sensor. The reusable MR safe probe connects to a console 22 which receives the light signal from the temperature sensor and converts the

signal to a human readable quantified measurement which is displayed on a display device 24 and/or used in conjunction with analysis of the received MR signals.

The display device 24 can be a separate device such as an LED display or incorporated into a workstation 26. The workstation 26 includes an electronic processor or electronic processing device 28, the display device 24, and at least one input device 30. The workstation 26 can be a desktop computer, a laptop, a tablet, a mobile computing device, a smartphone, and the like. The display device 24 can include a computer monitor, a touch screen, Cathode ray tube (CRT), Storage tube, Flat panel display, Light-emitting diode (LED) displays, Electroluminescent display (ELD), Plasma display panels (PDP), Liquid crystal display (LCD), Organic light-emitting diode displays (OLED), a projector, and the like. The input device 30 can be a keyboard, a mouse, a microphone, and the like.

The reusable MR safe probe 2 can be configured to receive and display light signals which correspond to a sensed value such as temperature as soon as connected to the console 22. The sensed value such as temperature can include a continuous measurement and the display on the display device 24 updated with the continuous measured values. The processor 28 can be configured with maximum or minimum values for the sensed values which sound an alarm such as an audible sound or visual display.

With reference to FIG. 2, one embodiment of a reusable MR safe probe 2 is schematically illustrated. The reusable MR safe probe 2 includes a fiber optic sensor probe 32 and a sheath 38. The fiber optic sensor probe 32 is shown with a distal portion 36 and a locking element 34 which engages the sheath 38 when the probe is inserted and indicates the proper depth in the sheath. The probe 32 is shown without the entire proximal portion and a connector. The probe 32 with the sheath 38 includes a maximum diameter which passes through a nasal passage of the subject such as 4.9 mm. The fiber optic sensor probe is reusable. The sheath is disposable. The sheath 38 covers and encloses the distal end of the probe and provides a non-permeable sterile surface.

The sheath in one embodiment includes tabs 40 at the proximal end of the sheath for pulling the sheath onto the probe 32 or holding the sheath while inserting the probe 32 to the indicated depth, and engaging the locking element 34. The tabs can be two opposing tabs which allow a healthcare practitioner to grasp the sheath and handle in a manner which maintains the sterile outer surface. Gripping the tabs and gripping the locking mechanism, opposing forces exerted by the healthcare practitioner can bring the proximal end of the sheath to the locking element and engage the sheath to the locking element, e.g. tightly couple the sheath to the locking element forming a pressure seal. The tabs 40 when pulled toward the distal end of the probe 32 and away from the locking element, assist the healthcare practitioner in removal of the sheath 38 from the probe 32. The sheath during removal can be pulled along the distal portion of the probe 32 by the tabs and fold the outer contaminated surface inside out. The removed sheath turned inside out can be safely handled and properly disposed.

The reusable MR safe probe 2, with the sheath 38 properly engaged with and enclosing distal end of probe 32 that includes the temperature sensor, is inserted into the esophagus or rectum of the subject. The reusable MR safe probe 2 with the sheath 38 and the probe 32 are inserted and removed from the subject as one unit. The sheath provides a sterile non-permeable barrier between the temperature sensing probe 32 and the subject.

In one embodiment, portions of the fiber optic sensor probe **32** and/or the sheath **38** can be manufactured with MR visible material, e.g. emits proton resonance for internal visual monitoring of the probe by the MR system. For example, a thin line in the sheath **38** can indicate the location and/or direction of the reusable MR safe probe **2** in an image reconstruction. The line can be a thin line, dotted line, include arrows, etc. The image reconstruction can show where the reusable MR safe probe **2** is internally in the subject. The portion of the MR visible material can be limited so that the material does not interfere with the image of the subject.

With reference to FIG. 3A, an embodiment of a fiber optic sensor probe **32** is shown in a perspective view. The locking element **34** divides the probe **32** into the distal portion **36** which includes a temperature sensor **42** and a proximal portion **44** which connects to console via a connector **46**. The distal portion **36** has a length of sterile surface such as 50.8-55.8 cm. The proximal portion **44** includes a length from the subject to the console such as 3-5.5 meters.

FIG. 3B shows an enlarged side view of fiber optic sensor probe **32**. The distal portion **36** includes a temperature sensor **42** and can include a rounded tip. The sensor operates from +20° C. to +44° C. ±0.5° C. The proximal portion **44** can include a polyvinyl-chloride (PVC) covered single optical fiber. The proximal portion can be colored blue for visibility. The proximal portion includes a connector **46** which can operate reliably after multiple insertion cycles and in one embodiment meets an IEC 61754 standard e.g. IEC 61754-4. The PVC material, such as DEHP free 85A grey PVC from Sunlight Corporation, produces no visible MR signal, e.g. invisible to MR imaging. The connector **46** connects to the system **1** via a fiber optic connector in the console **22** and can include standard fiber optic connector interfaces. FIG. 3C shows an end view of the connector **46**. The single optical fiber **48** is enclosed with the connector and optically connects to the console such that light communication is provided between the temperature sensor **42** and the console **22**.

With reference to FIG. 3D, a side view of the locking element **34** is shown in a central slice. The locking element includes a rigid tapered surface **50**. The locking element can include marks **52** in the surface and/or lines which indicate the proper distance for insertion of the probe **32** into the sheath **38**. The locking element includes a maximum outer diameter which is large the maximum inner diameter of the sheath **38**. The length of the locking element can include a length easily gripped by the healthcare practitioner such as 5 cm. The size can be limited by the bulk and weight in handling of the probe by the healthcare practitioner. FIG. 3E shows a cross section view of the locking element **34** with the enclosed single optical fiber **48**. Although a single optical fiber for both transmitted and returned light is illustrated, separate transmit and return optical fiber are also contemplated. Further, additional optical fibers may transmit light to and from other biological sensors.

FIG. 4 illustrates an embodiment of the sheath **38** in perspective. The sheath **38** includes a material which produces no MR signal such as TSP 1051-85A polyurethane made by Polyzen. The material emits no proton resonance, e.g. invisible to MR imaging. The material encloses the distal portion **36** of the probe **32**, as shown in reference to FIG. 2, in a cavity with one opening and carries the probe **32** within the cavity or opening of the sheath **38**. The sheath can be further divided into a proximal portion **54**, a central portion **56**, and a distal portion **58**. The central portion and

distal portion provides flexibility and sufficient strength with a thickness such as 0.0381 mm.

The distal portion **58** can include a rounded tip **60**. The rounded tip can ease the insertion into the subject as the probe bends and moves through the narrow nasal passage of the subject. The rounded tip can conform to a rounded tip of the probe **32** or provide a rounded tip to the probe **32**. The distal portion **58** can include a length such as 20.3 cm with a smaller outer diameter such as 3.9 mm.

The central portion **56** can include a slightly larger outer diameter such as 4.9 mm for a length such as 30.5 cm. The central portion **56** and the distal portion **58** provide an overall length of a sterile outer surface such as 50.8 cm.

The proximal portion **54** includes a rigid or thickened tubular connection **62** to the central portion. The proximal portion includes an outer diameter with firmness and tear resistance to engage the tapered locking element **34** of the fiber optic sensor probe **32** such as 6.04 mm. The proximal portion extends for a length such as 25.4 mm which provides sufficient area to engage the locking element **34**.

Two opposing flaps or tabs **40** connect to the proximal end **64** of the proximal portion **54**. The tabs extend for a length such as 2.5 cm with a flare such as 9.4 mm for easy gripping by the healthcare practitioner. For example, the healthcare practitioner can grip the proximal end of the locking element **34** of the probe **32** in one hand and grip a tab either side of the sheath in the other. Using opposing forces the sheath can be drawn onto the distal end of the probe **32** or the sheath can be held stationary while the distal end of probe **32** is pushed into the sheath. The proximal portion **54** is pulled by the tabs onto the tapered surface **50** of the locking element **34** to be stretched in a friction locking interaction.

FIG. 5 illustrates an embodiment of the sheath **38** with an optional cover **66** in a cross section view. The sheath includes at least one perimeter seam **68**. The perimeter seam is formed to the outside surface. In one embodiment, two perimeter seams are formed opposite. The perimeter seams seal the material of the sheath to provide a sterile outer surface **70**. The optional cover **66** such as a peel away introducer with a sterile inner surface can be for an individual sheath. The perimeter seam formed to the outside includes an air channel **72** on the inside which allows air to escape during insertion. By allowing the air to escape, a potential thermal barrier of trapped air is eliminated. A thermal barrier of trapped air can affect the temperature reading by the sensor **42**. The at least one perimeter seam also forms the cavity **74** which carries the distal portion of the probe **32** and includes the central **56** and distal **58** portions of sheath **38**.

With reference to FIG. 6 an embodiment of the reusable MR safe probe **2** with a surface application is illustrated. The distal portion of the probe **32** is fully inserted into the sheath **38** and the locking element **34** engages the proximal portion **54** of the sheath **38**. The tabs **40** extend over the locking element. An applicator **76** such as an adhesive backed biocompatible material is applied over the tip of the reusable MR safe probe **2** and affixed to the skin surface of the subject **6**. During removal, the applicator **76** and the sheath **38** can be disposed of as a unit. By using the sheath, any adhesive adheres to the sheath **38** and not the surface of the probe **32**, which avoids potential damage with the removal of any adhesive from the reusable probe **32**.

FIGS. 7A-7M diagrammatically illustrate various embodiments of the reusable MR safe probe **2**. In FIG. 7A, the probe **32** and the sheath **38** include a stepped locking element. The distal end of the sheath has mating steps which frictionally engage the steps of the locking element. FIG. 7B

shows a tapered locking element of both the probe 32 and the sheath 38. The tapered locking element on the probe 32 expands to a larger diameter than the tapered locking element located on the proximal end of the sheath 38. The tapered locking element located on the proximal end of the sheath engages frictionally the tapered locking element of the probe. A barbed locking element on the probe 32 is shown in FIG. 7C. The straight or flared sheath 38 slides over the barbed locking element on the probe and engages with the barbed locking element with friction. A plastic collet 78 on the probe 32 in FIG. 7D engages and holds the sheath 38. A locking ring 80 clamps the collet tight around the proximal edge of the sheath. The locking ring slides from the proximal towards the distal end to lock the collet. The sheath 38 is rolled onto the probe 32 using a draw string 82 in FIG. 7E. The sheath is rolled by pulling the draw string towards the proximal end of the probe and unrolls the sheath with a tight fit onto the probe. A locking element is threaded on the probe 32 and the sheath 38 in FIG. 7F. The probe is inserted into the sheath and with a twisting motion such as with a screw, the female portion located on the sheath engages the male portion locking element of the probe. In FIG. 7G, a barbed locking element is included in the sheath 38. The probe is inserted into the sheath and pulled with the locking element of the sheath frictionally engaging the straight surface of the probe. The sheath 38 includes the plastic collet in FIG. 7H. A locking ring 84 slides over the plastic collet incorporated into the proximal end of the sheath. The ring slides from the distal to the proximal end. The sheath 38 includes a crushable band in FIG. 7I. The probe includes a rough surface which frictionally engages the sheath after crushing. The sheath 38 includes one or more tails in FIG. 7J which are tied around the probe 32. The sheath is pulled over the probe and the tails are tied around the probe to hold the sheath in position. The sheath 38 includes a length of decreased diameter near the tip which prevents the sensor 42 on the distal portion of the probe 32 from slipping out in FIG. 7K. The sheath is pulled onto the probe and the remainder of the sheath can be increased in thickness which increases the rigidity of the remaining portion. The sheath 38 in FIG. 7L includes a flange to assist gripping by the healthcare practitioner during insertion of the probe 32 into the sheath. The flange provides a rigid surface which extends radially from the proximal end of the sheath. The sheath 38 in FIG. 7M includes a cover 66 such as a peel away introducer. The introducer includes tabs which provide a gripping surface. The healthcare practitioner grasps the tabs and pulls the sheath onto the probe. After the probe is fully inserted into the sheath, the introducer is peeled away leaving the sheath covering the distal end of the probe.

With reference to FIG. 8 one method of configuring the reusable MR safe probe 2 for insertion into a subject 6 is flowcharted. In a step 86, the probe 32 is uncoiled. The uncoiling avoids knotting or kinking the probe 32. In a step 88, the healthcare practitioner examines the probe 32 for damage, adhesives or residue.

In a step 90, the healthcare practitioner inserts the probe 32 into the sheath 38. The healthcare practitioner holds the tabs 40 of the sheath 38 and pulls the sheath completely over the distal portion 36 of the probe 32 until the locking element 34 of the probe 32 is fully seated into or engaged with the proximal end 64 of the sheath 38 and the two opposing tabs 40 rest over the locking element 34. In embodiments with an additional locking element, the locking element is engaged when the sheath is properly seated, the distal portion of the probe 32 fills the sheath completely

to the tip, e.g. no open cavity with air at the end of the sheath. The step can include removal of an optional cover 66 such as a peel away introducer. The reusable MR safe probe 2 is connected to the system 1 via the console 22 with the connector 46 in a step 92. Connecting to the console 22 can initiate sensor or specifically temperature readings. In an optional step 94, surgical tape can be applied to the tabs 40 and around the locking element 34.

The reusable MR safe probe 2 with a sterile outer surface is inserted into the subject 6, e.g. through a nasal passage or rectum in a step 96. The probe 2 provides sensor readings with light communications via an optical fiber 48 using a non-ferrous sensor 42 and does not include conductive elements such as ferrous sensors or conductive wires. The absence of conductive elements such as ferrous sensors or conductive wires eliminates the potential hazard of burns to the subject. The material of the probe 2 produces no MR signal, e.g. invisible to MR imaging, which eliminates potential distortions or gaps in imaging. The biocompatible sterile outer surface of the probe 2 allows usage internally to a subject 6.

FIG. 9 flowcharts one method of removing the sheath 38 from the reusable MR safe probe 2. In a step 98, surgical tape is removed from around the tabs 40 if surgical tape was previously applied. The sheath is removed in a step 100. The healthcare practitioner grips the tab or tabs 40 of the sheath 38, and the proximal end of the locking element 34 of the probe 32. With opposing force the sheath 38 is pulled from the probe 32 while turning the contaminated outer surface of the sheath 38 inside out. In a step 102, the sheath is properly discarded according to a facility's biohazard procedures.

In a step 104, the probe 32 is inspected by the healthcare practitioner, which ensures that the sheath was completely removed from the probe 32. The probe 32 is cleaned and/or disinfected in a step 106.

With reference to FIG. 10 one method of configuring the reusable MR safe probe 2 for a surface application is flowcharted. In a step 108, the healthcare practitioner cleans and dries the application site on the subject 6. In a step 110, the healthcare practitioner inserts the fiber optic sensor probe 32 into the cavity of the sheath 38 by gripping the tabs 40 and pulling the sheath onto the distal portion of probe 32 until fully engaged by the locking element 34 of the probe 32.

The healthcare practitioner positions the sensing tip of the reusable MR safe probe 2 at application site of the subject 6 in a step 112. The backing is removed from an applicator 76 in a step 114. The applicator 76 with the backing removed is applied over the sensing tip of the reusable MR safe probe 2 at application site of the subject 6 in a step 116.

It is to be appreciated that in connection with the particular illustrative embodiments presented herein certain structural and/or function features are described as being incorporated in defined elements and/or components. However, it is contemplated that these features may, to the same or similar benefit, also likewise be incorporated in other elements and/or components where appropriate. It is also to be appreciated that different aspects of the exemplary embodiments may be selectively employed as appropriate to achieve other alternate embodiments suited for desired applications, the other alternate embodiments thereby realizing the respective advantages of the aspects incorporated therein.

It is also to be appreciated that particular elements or components described herein may have their functionality suitably implemented via hardware, software, firmware or a combination thereof. Additionally, it is to be appreciated that

certain elements described herein as incorporated together may under suitable circumstances be stand-alone elements or otherwise divided. Similarly, a plurality of particular functions described as being carried out by one particular element may be carried out by a plurality of distinct elements acting independently to carry out individual functions, or certain individual functions may be split-up and carried out by a plurality of distinct elements acting in concert. Alternately, some elements or components otherwise described and/or shown herein as distinct from one another may be physically or functionally combined where appropriate.

In short, the present specification has been set forth with reference to preferred embodiments. Obviously, modifications and alterations will occur to others upon reading and understanding the present specification. It is intended that the invention be construed as including all such modifications and alterations insofar as they come within the scope of the appended claims or the equivalents thereof. That is to say, it will be appreciated that various of the above-disclosed and other features and functions, or alternatives thereof, may be desirably combined into many other different systems or applications, and also that various presently unforeseen or unanticipated alternatives, modifications, variations or improvements therein may be subsequently made by those skilled in the art which are similarly intended to be encompassed by the following claims.

What is claimed is:

1. A magnetic resonance probe configured for both insertion into and application to a surface of a subject, the magnetic resonance probe comprising:
 - a reusable fiber optic sensor probe comprising:
 - a distal portion having a sensor end and a locking element end opposite from the sensor end;
 - a proximal portion;
 - a locking element connecting the locking element end of the distal portion to the proximal portion, wherein the locking element comprises a tapered rigid surface and an indicator that indicates a proper distance for sheath insertion;
 - a non-ferrous sensor on the sensor end of the distal portion; and
 - an optical fiber connected with the non-ferrous sensor, the optical fiber extending from the proximal portion to the non-ferrous sensor;
 - a disposable sheath having a non-permeable sterile outer surface, a closed end and an open end opposite from the closed end, wherein the closed end covers the sensor end of the fiber optic sensor probe so that the distal portion of the fiber optic sensor probe fills the sheath, wherein the open end of the sheath comprises pull tabs, and wherein a portion of the open end of the sheath engages with the locking element at or near the indicator; and
 - a removable applicator configured to affix the closed end of the sheath to a surface of a subject.

2. The magnetic resonance probe according to claim 1, wherein the closed end of the sheath comprises a rounded tip.

3. The magnetic resonance probe according to claim 1, wherein the sheath further comprises:

at least one perimeter seam located on the outside of the sheath which provides enclosure of a central portion and a distal portion of the sheath about a cavity which carries the distal portion of the fiber optic sensor probe.

4. The magnetic resonance probe according to claim 1, wherein the pull tabs are configured to allow a healthcare practitioner to remove the sheath from the fiber optic sensor probe while turning a central portion and a distal portion of the sheath inside out.

5. The magnetic resonance probe according to claim 1, wherein the material of the fiber optic sensor probe and the sheath produce minimal magnetic resonance signal.

6. The magnetic resonance probe according to claim 1, wherein the non-ferrous sensor includes a temperature sensor configured to measure a temperature change from 20 C-37 C in 20 seconds or less.

7. The magnetic resonance probe according to claim 1, wherein

the sheath includes a tube of a material which produces no magnetic resonance signal.

8. The magnetic resonance probe according to claim 7, wherein the tube comprises:

a tubular proximal portion connected to the open end of the material which engages and connects with a locking element of the sensor probe.

9. The magnetic resonance probe according to claim 7, wherein the material comprises at least one perimeter seam which runs the length of the cavity on the outside of the cavity and provides an air channel on the inside of the at least one perimeter seam.

10. The magnetic resonance probe according to claim 7, wherein the sheath is at least 50.8 cm long and less than 4.9 mm in diameter.

11. The magnetic resonance probe according to claim 7, further comprising:

a removable cover which covers and maintains the sterile outer surface of the material.

12. The magnetic resonance probe according to claim 7, wherein the sheath engages the probe with a tapered friction fit.

13. The magnetic resonance probe of claim 7, wherein: the fiber optic sensor probe comprises a fiber optic temperature sensing catheter including a temperature sensing probe and an elongated shaft carrying at least one optical fiber.

14. The magnetic resonance probe of claim 13, wherein the elongated shaft has one or more magnetic resonance visible markings.

* * * * *

专利名称(译)	可重复使用的MR安全温度探头，用于表面和体温测量		
公开(公告)号	US10631736	公开(公告)日	2020-04-28
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[标]申请(专利权)人(译)	皇家飞利浦电子股份有限公司		
申请(专利权)人(译)	皇家飞利浦N.V.		
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[标]发明人	ONEILL FRANCIS PATRICK KOVALSKY LEONARD JOHN IVANOV IVARS KASPICK STEVEN ANDREW GEMMATI MICHAEL JIRKA KEVIN WEINACHT JOHN BORNE FREDERIC EMMANUEL VACHON SAVARY MAXIM		
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摘要(译)

磁共振探头2包括光纤传感器探头32和护套38。光纤传感器探头32包括在配置为插入对象中的远端部分36上的非铁质传感器42，连接到远端部分的锁定元件34。36和连接到锁定元件34并通过光纤48与有色金属传感器42光连通的近端部分44和 包括一个连接器(46)。护套38覆盖光纤传感器探头32的远端部分36，与锁定元件34接合，并提供无菌的外表面70。

