

US010010258B2

(12) **United States Patent**
Bunch et al.

(10) **Patent No.:** **US 10,010,258 B2**
(45) **Date of Patent:** ***Jul. 3, 2018**

(54) **ATRIAL FIBRILLATION TREATMENT SYSTEMS AND METHODS**

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(*) Notice: Subject to any disclaimer, the term of this patent is extended or adjusted under 35 U.S.C. 154(b) by 0 days.

This patent is subject to a terminal disclaimer.

(21) Appl. No.: **15/047,670**

(22) Filed: **Feb. 19, 2016**

(65) **Prior Publication Data**
US 2016/0166166 A1 Jun. 16, 2016

Related U.S. Application Data

(63) Continuation of application No. 13/923,348, filed on Jun. 20, 2013, now Pat. No. 9,295,399.

(60) Provisional application No. 61/662,323, filed on Jun. 20, 2012, provisional application No. 61/799,242, filed on Mar. 15, 2013, provisional application No. 61/798,456, filed on Mar. 15, 2013.

(51) **Int. Cl.**
A61B 5/046 (2006.01)
A61B 5/00 (2006.01)
A61B 5/04 (2006.01)

(52) **U.S. Cl.**
CPC **A61B 5/046** (2013.01); **A61B 5/04012** (2013.01); **A61B 5/6869** (2013.01); **A61B 5/7264** (2013.01)

(58) **Field of Classification Search**
CPC A61B 5/04525; A61B 5/046; A61B 5/7264
See application file for complete search history.

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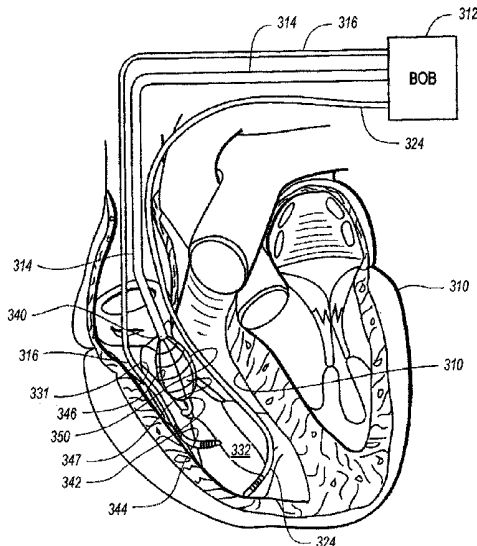
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(57) **ABSTRACT**

Methods for treating cardiac complex rhythm disorder in a patient can include receiving a plurality of electrical signals from a sensor system, wherein each electrical signal corresponds with a separate location on a cardiac wall of the heart of the patient, and wherein each electrical signal comprises an electrogram waveform; and ranking the electrical signals relative to each other based on at least a uniformity and a frequency of the electrogram waveform of each electrical signal.

41 Claims, 54 Drawing Sheets



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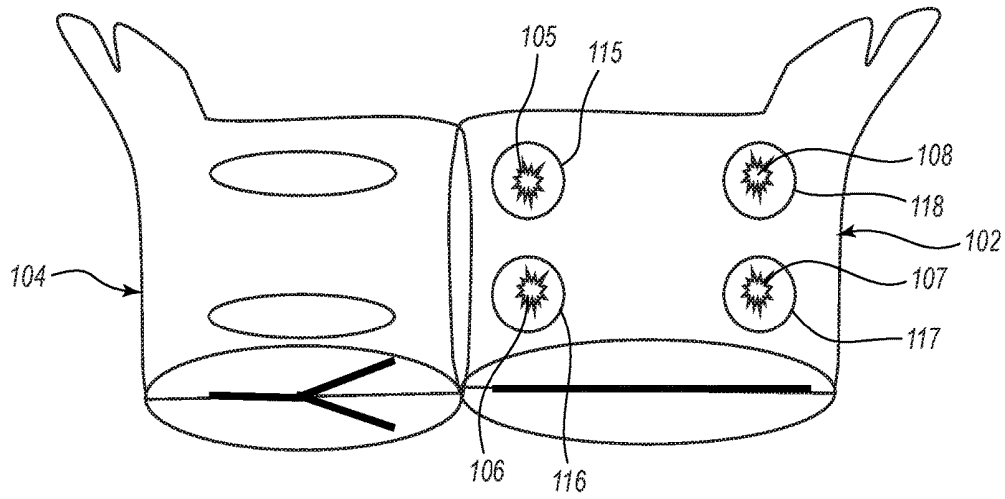


FIG. 1

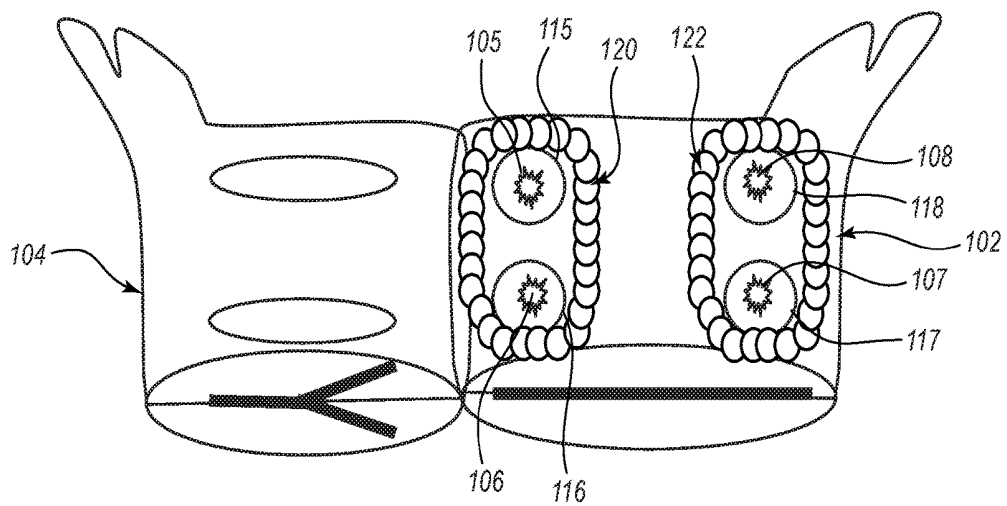


FIG. 2

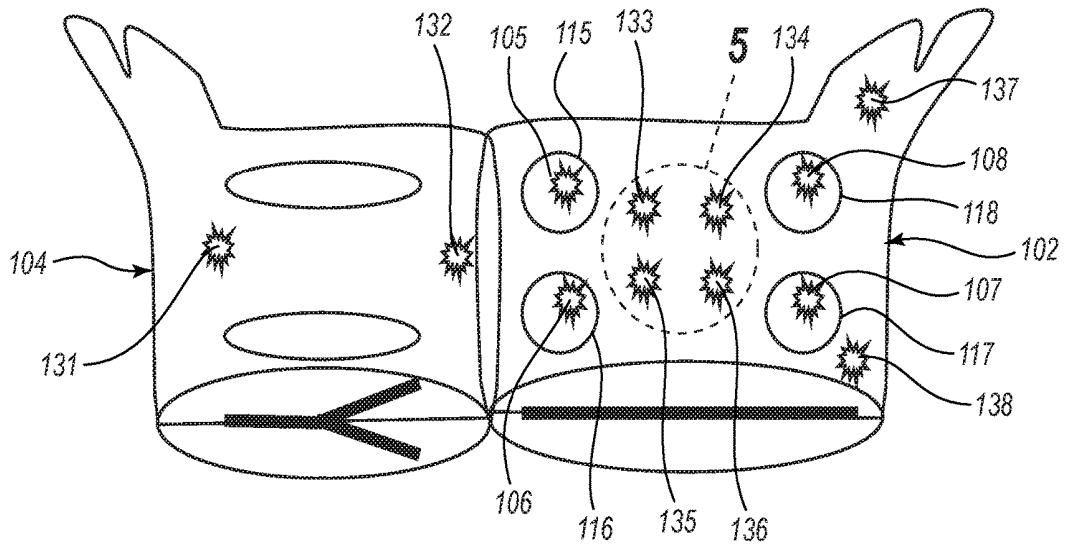


FIG. 3

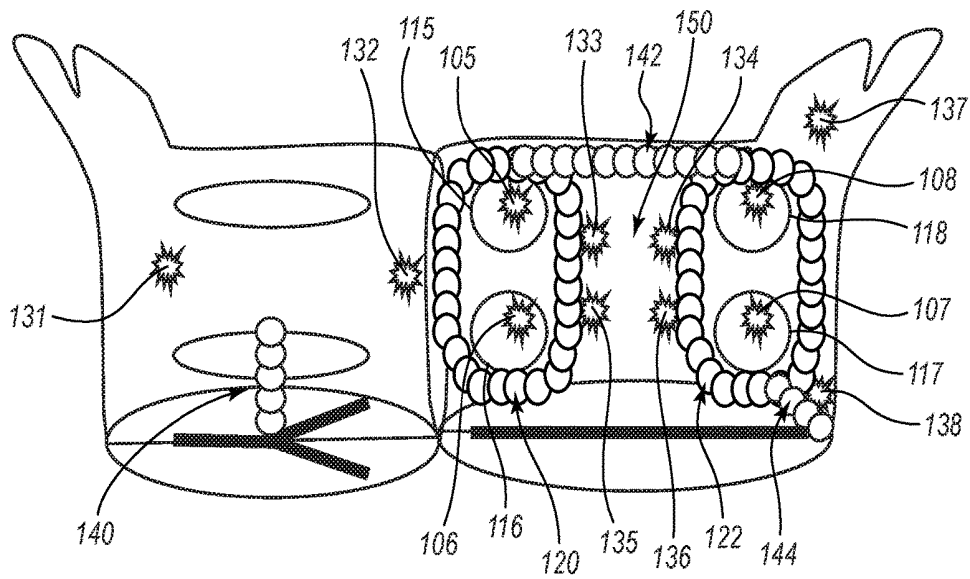


FIG. 4

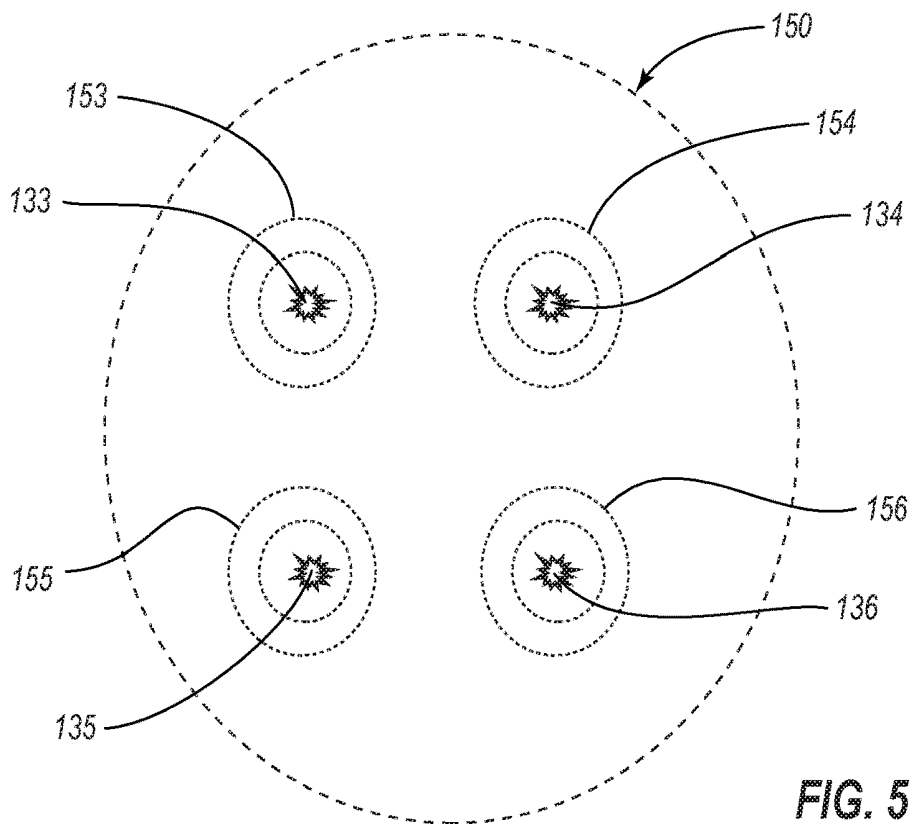


FIG. 5

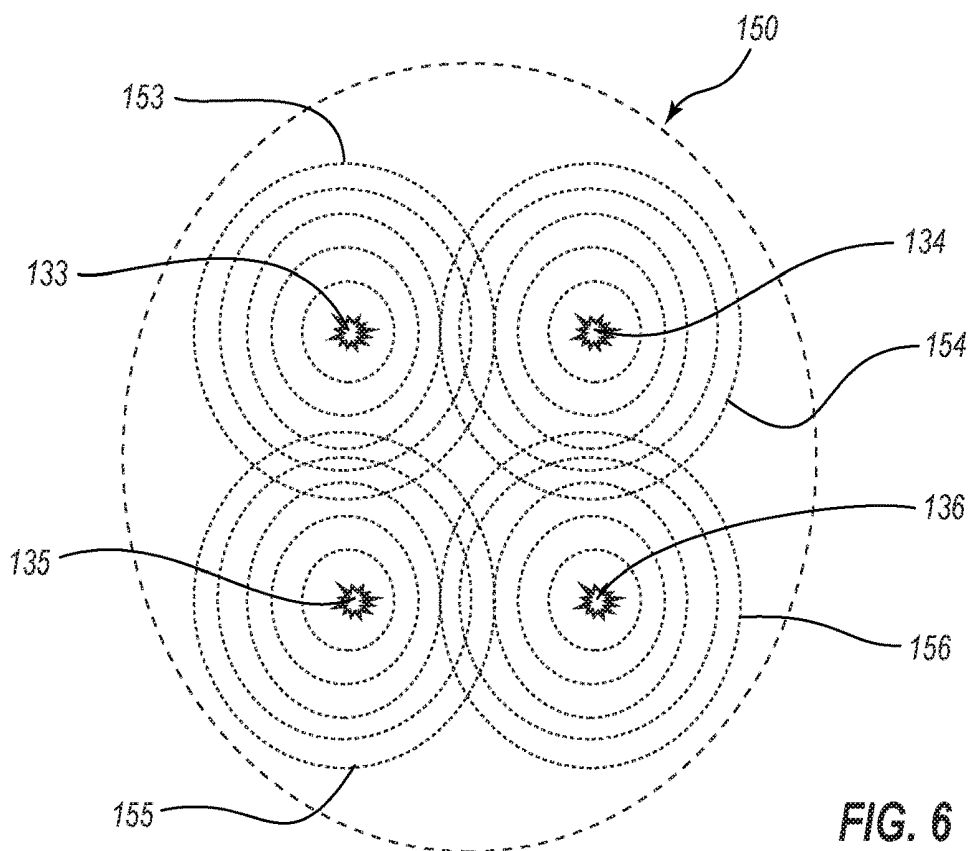


FIG. 6

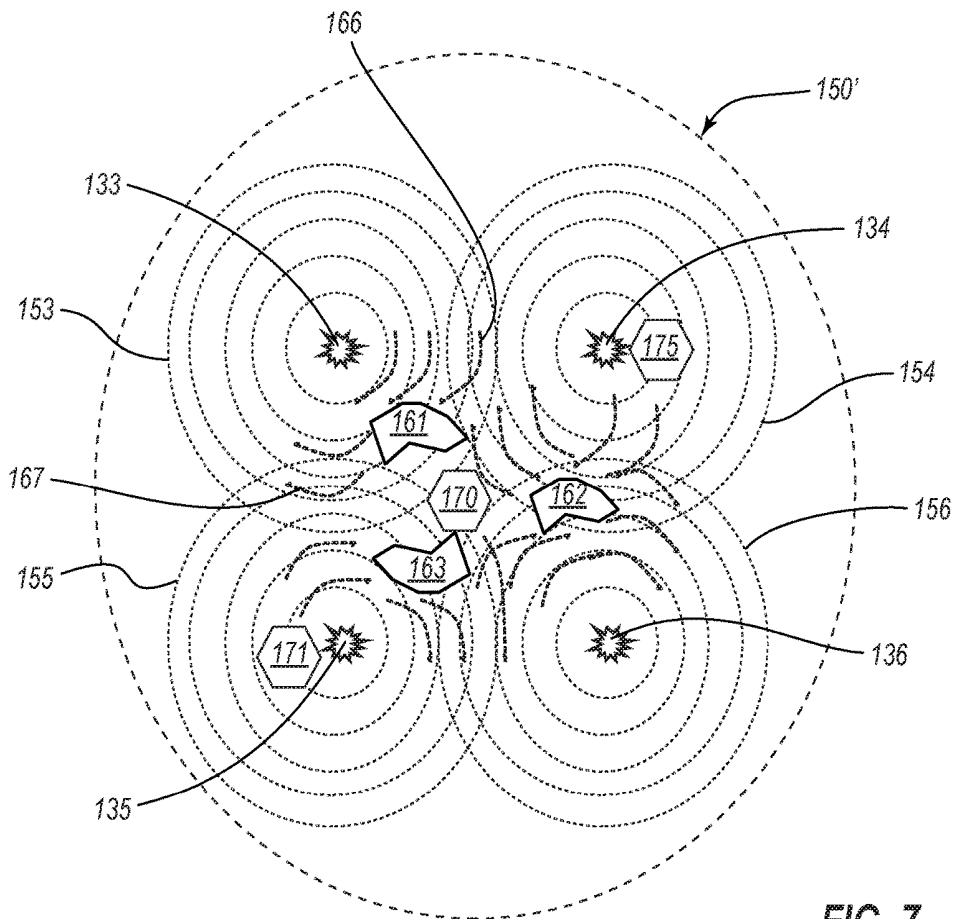


FIG. 7

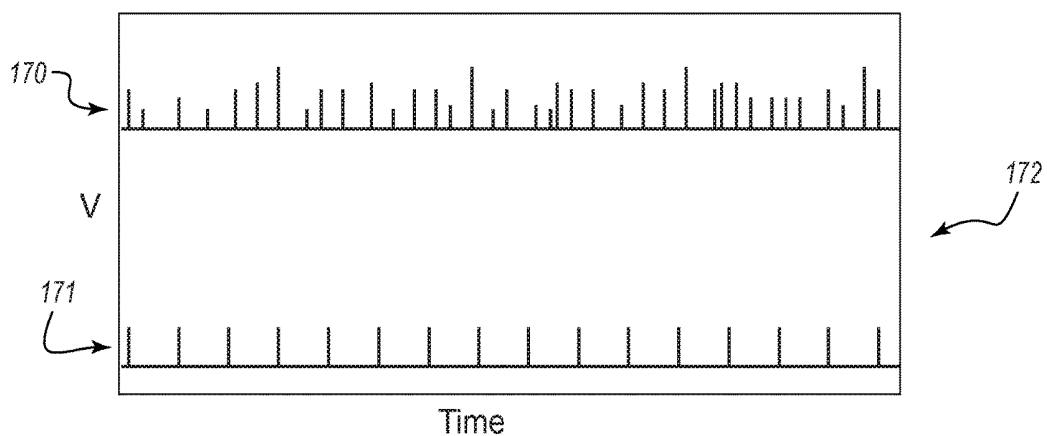


FIG. 8

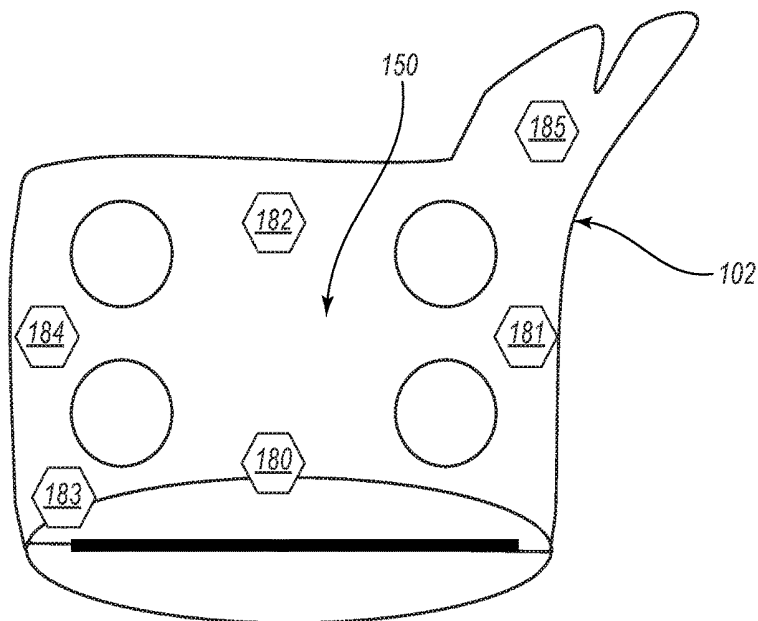
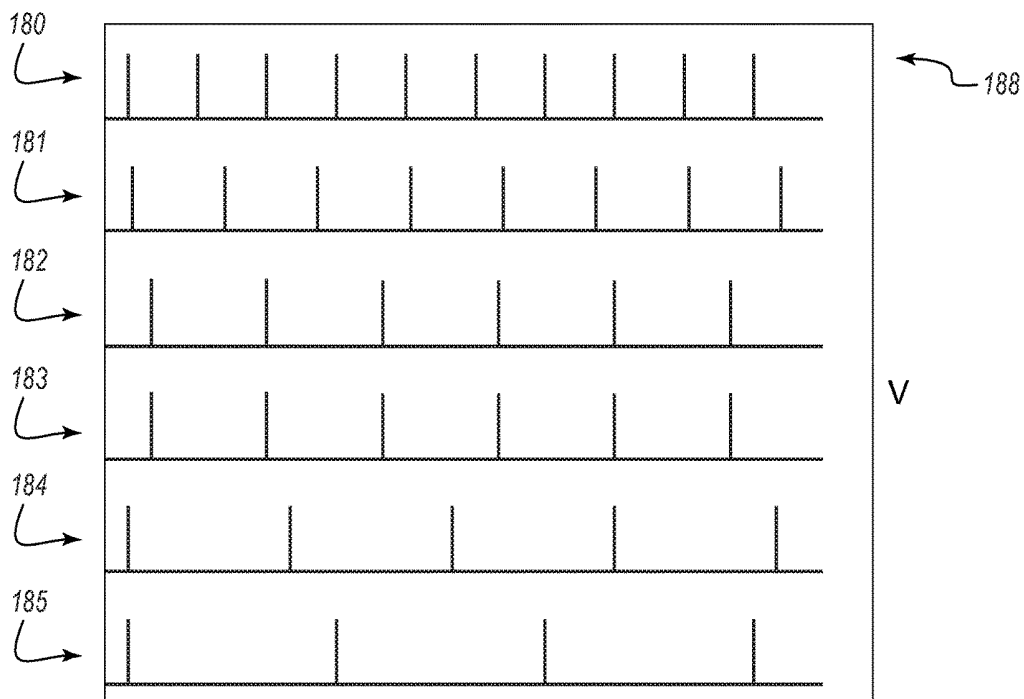


FIG. 9



Time

FIG. 10

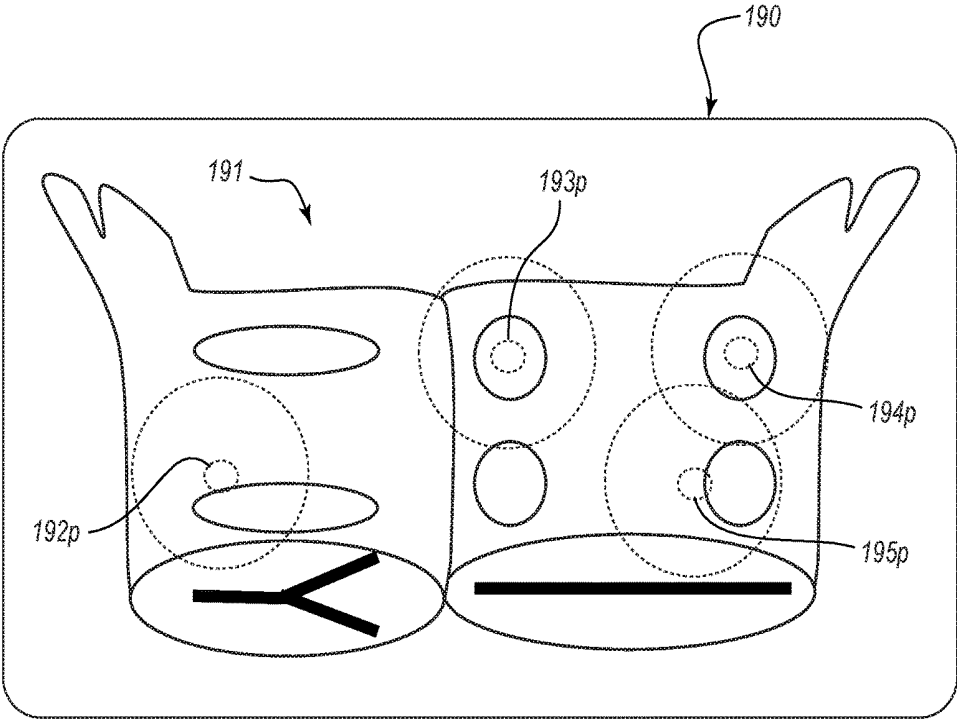


FIG. 11

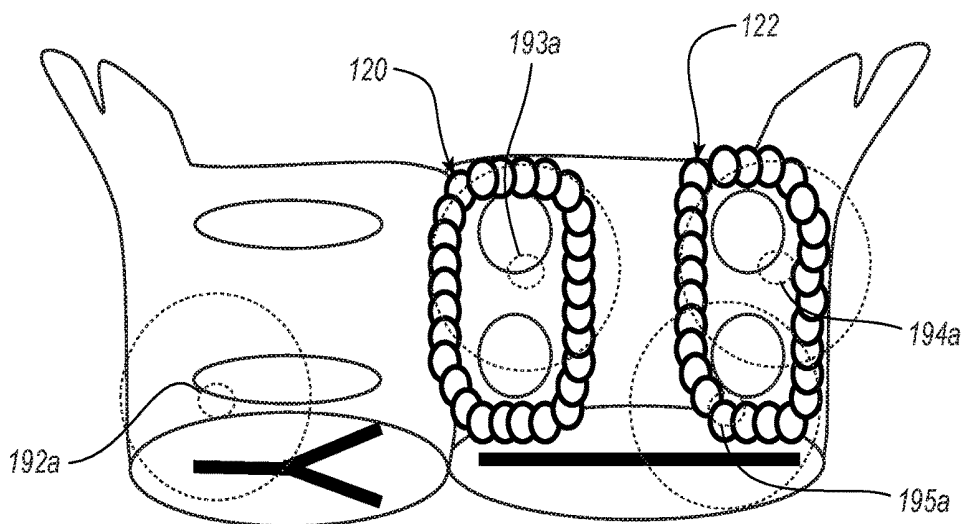


FIG. 12

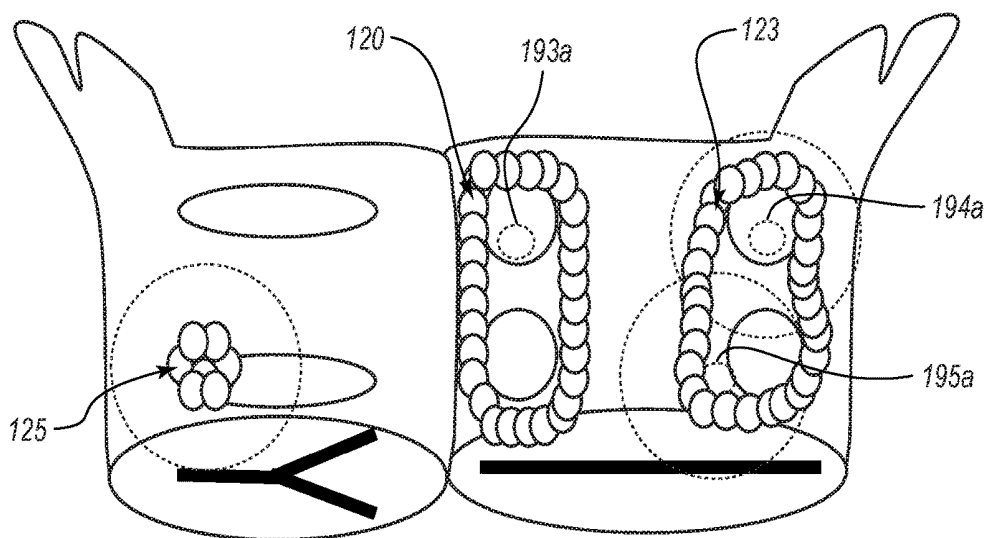


FIG. 13

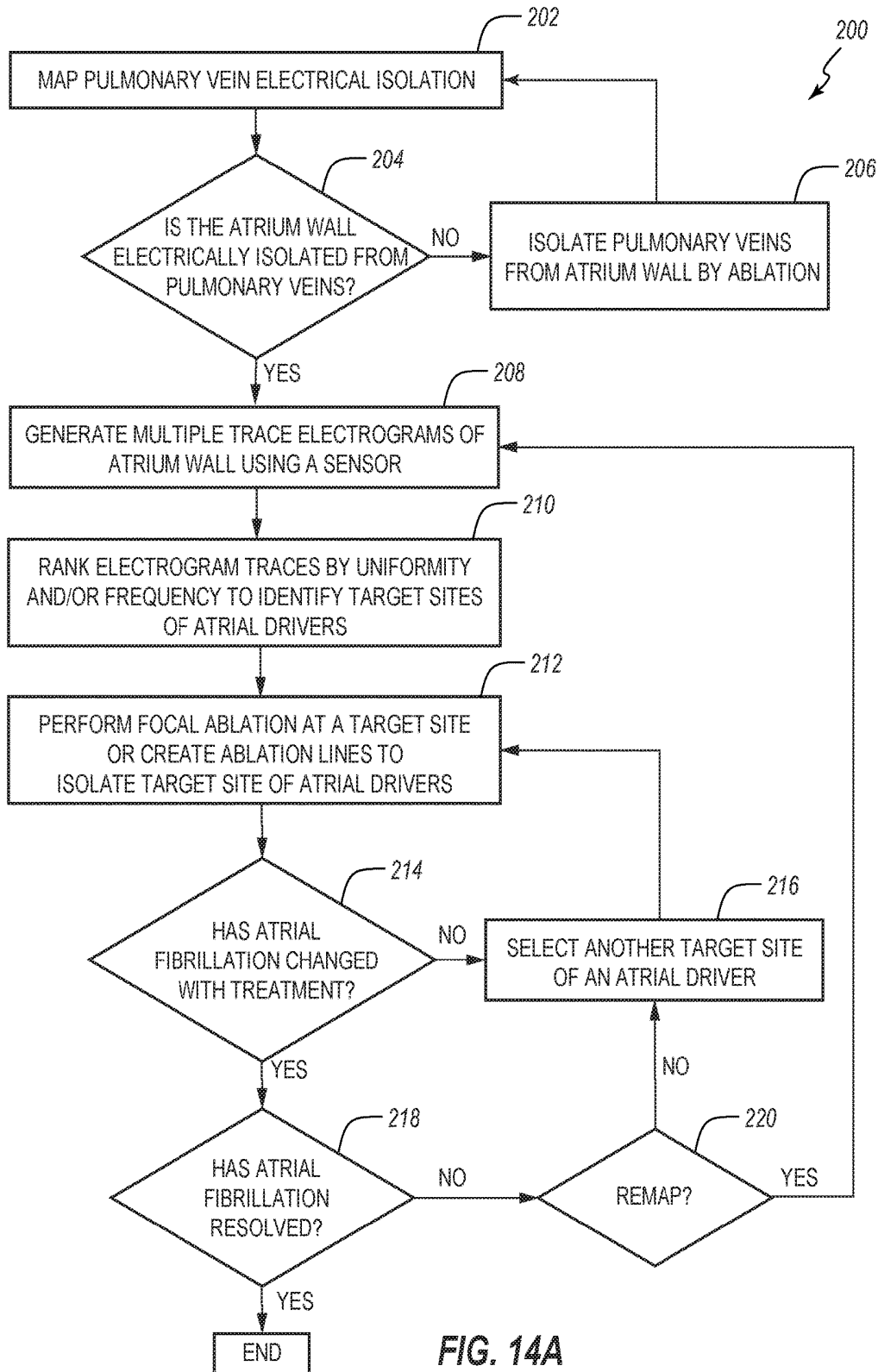


FIG. 14A

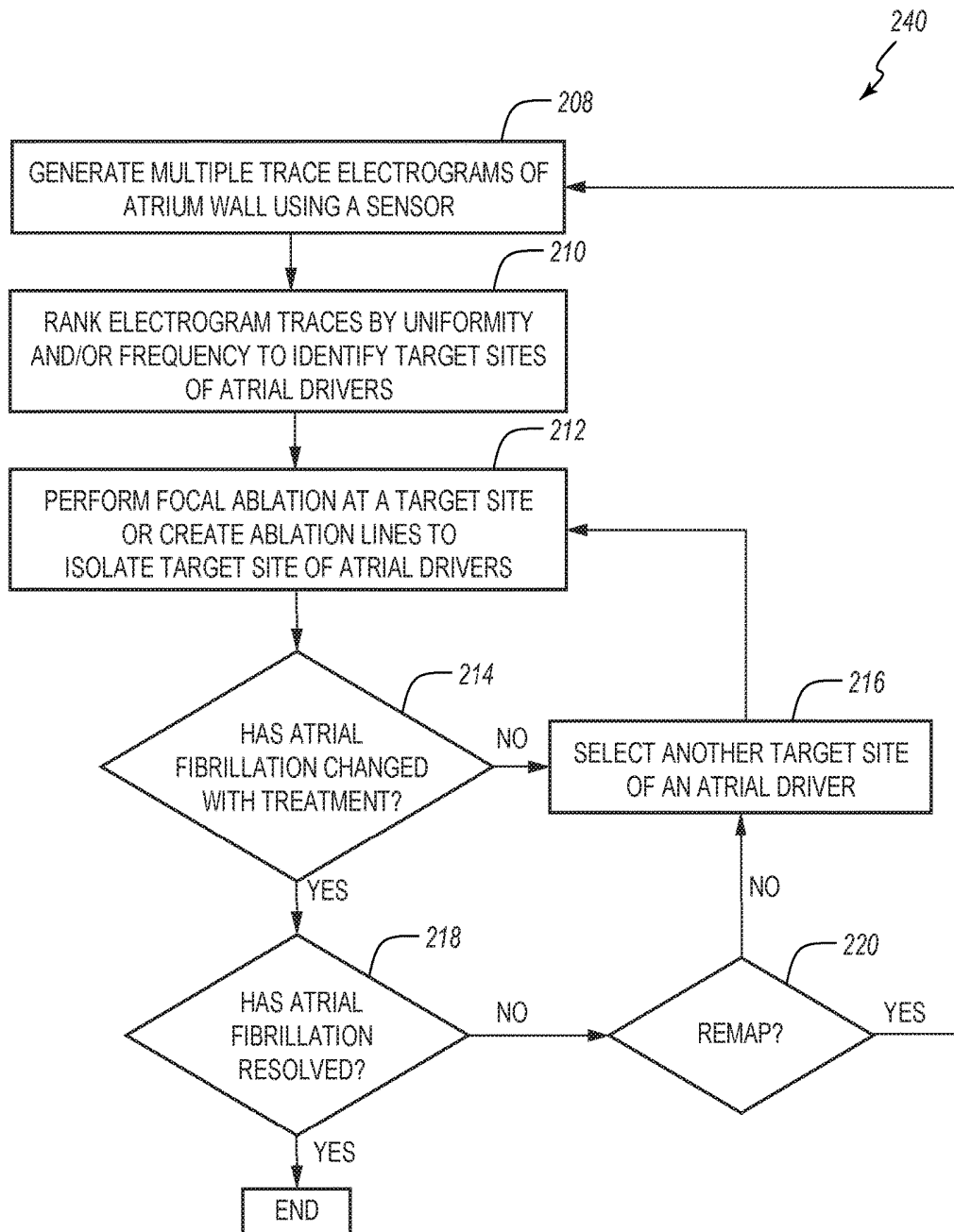


FIG. 14B

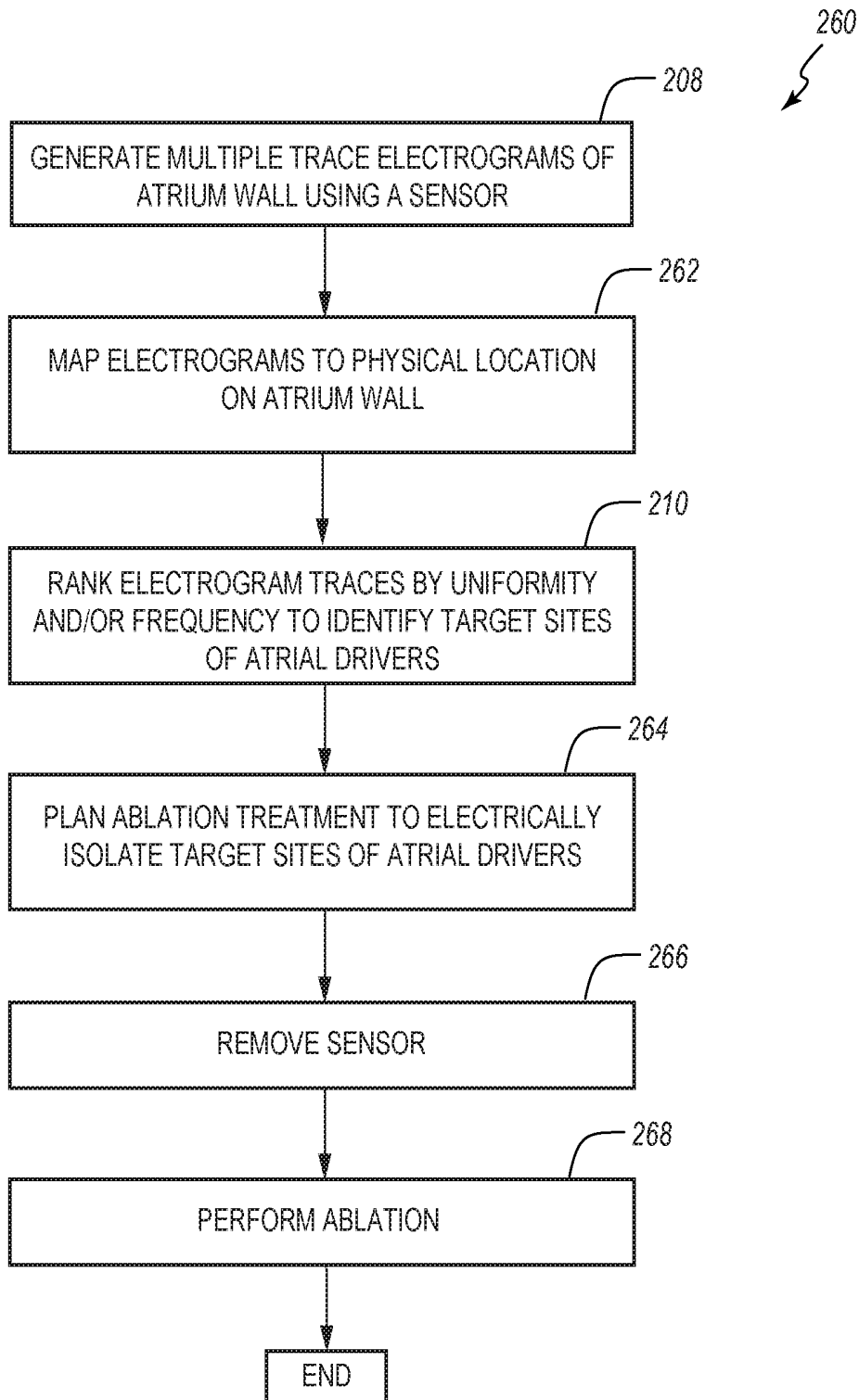


FIG. 14C

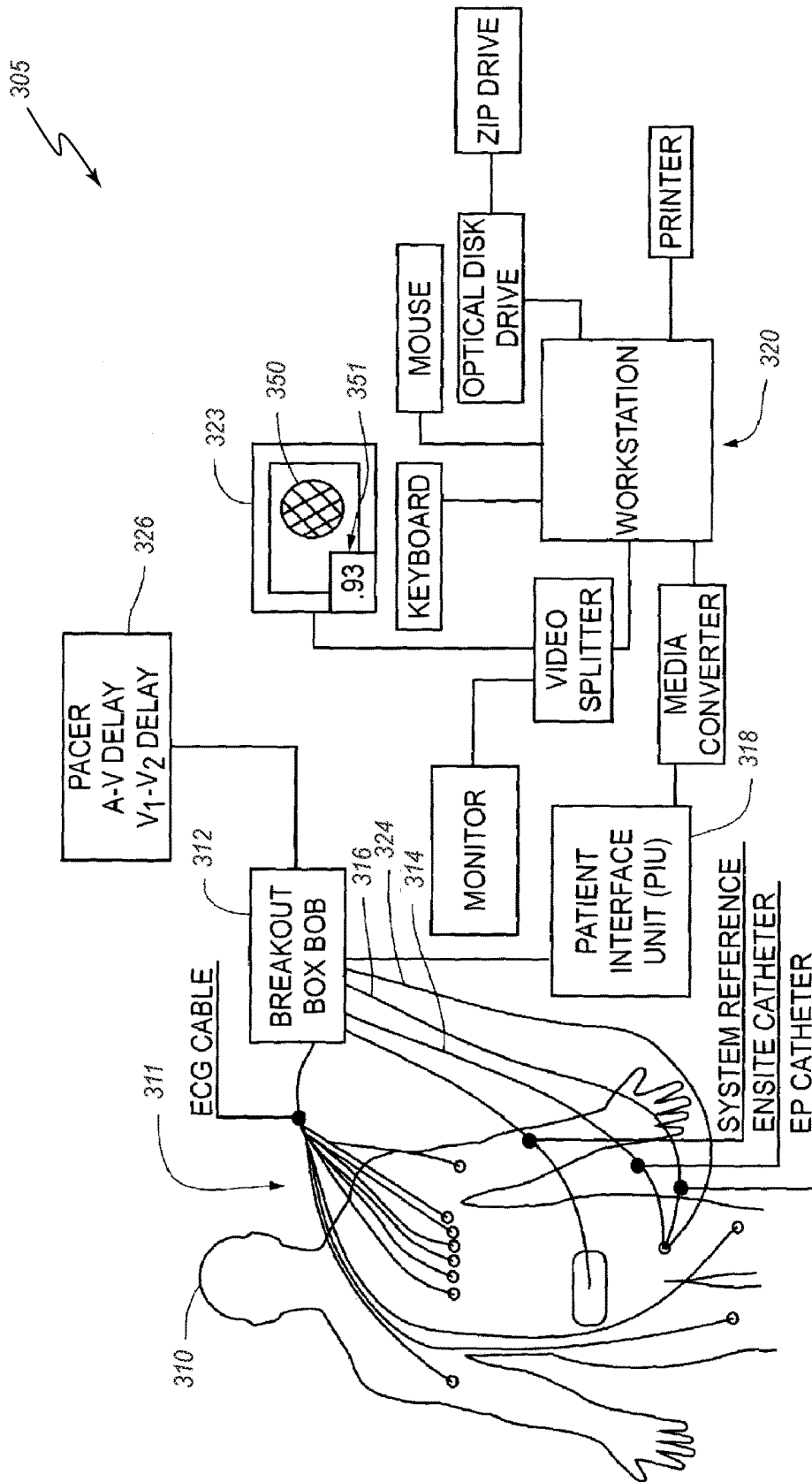


FIG. 15

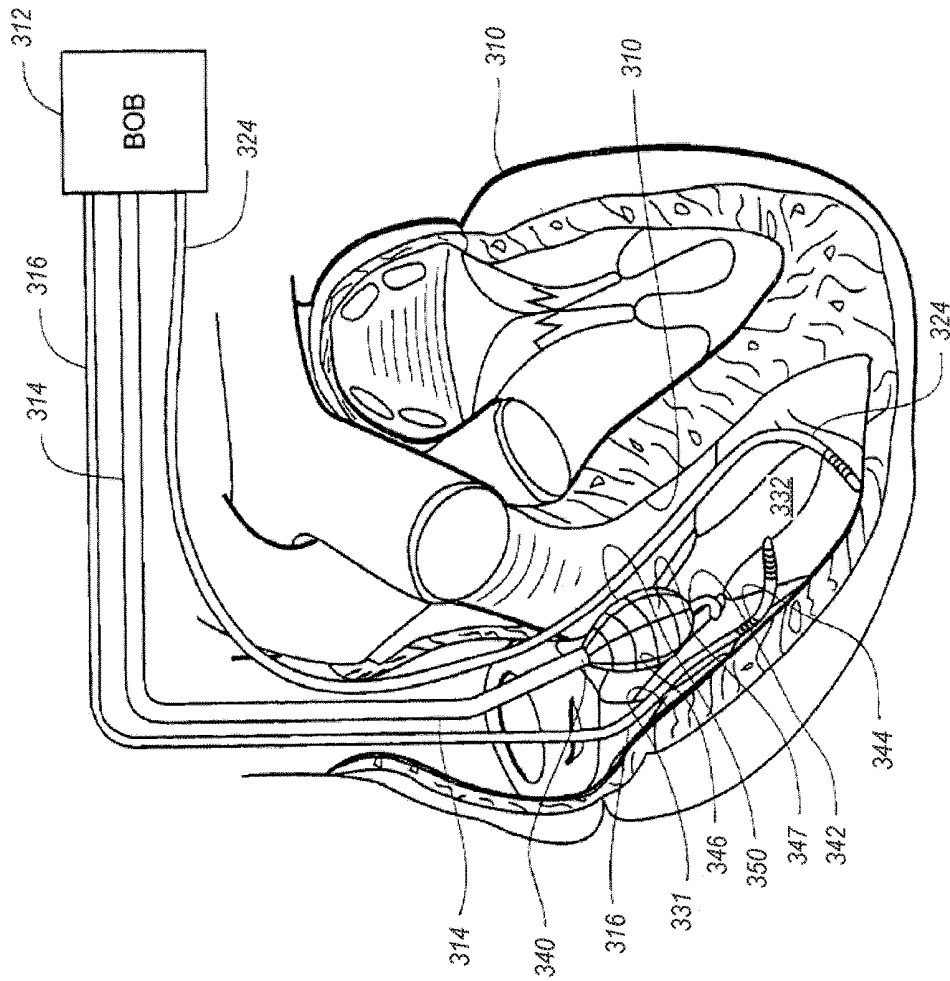


FIG. 16

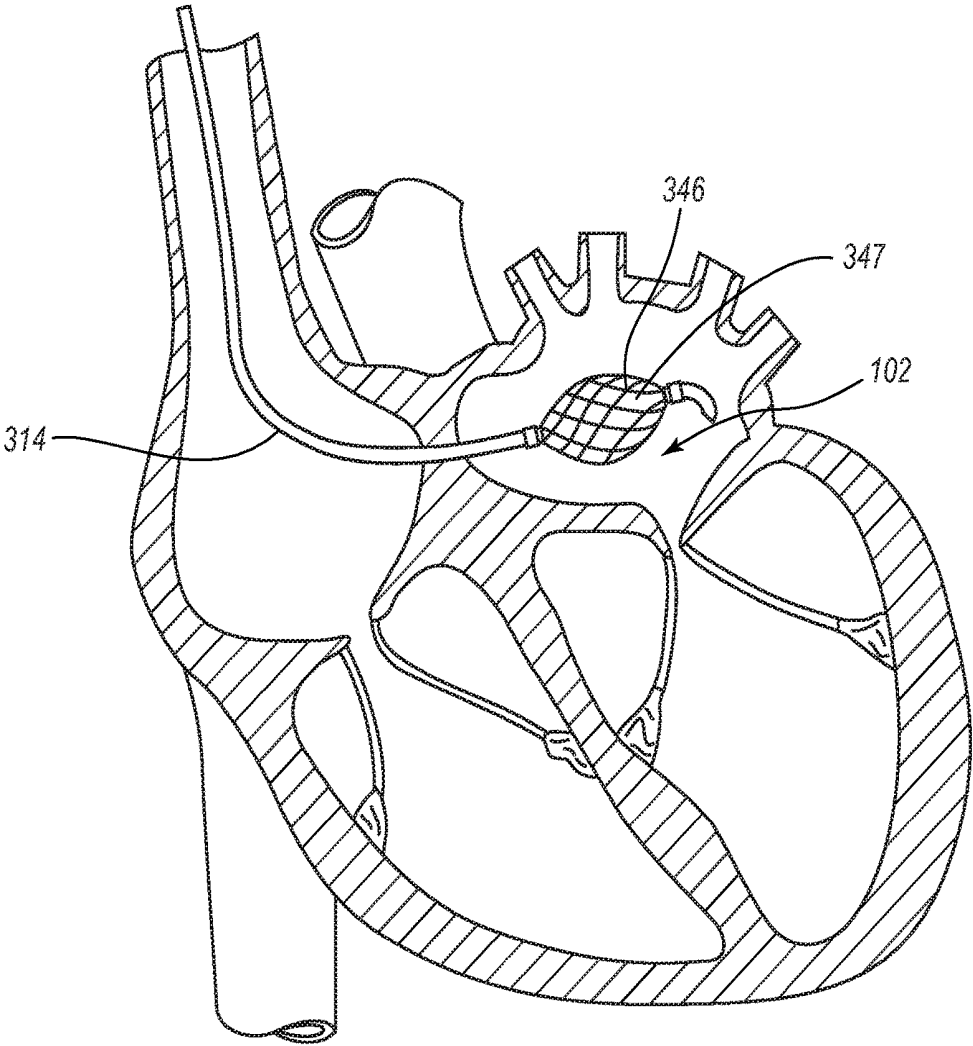


FIG. 17

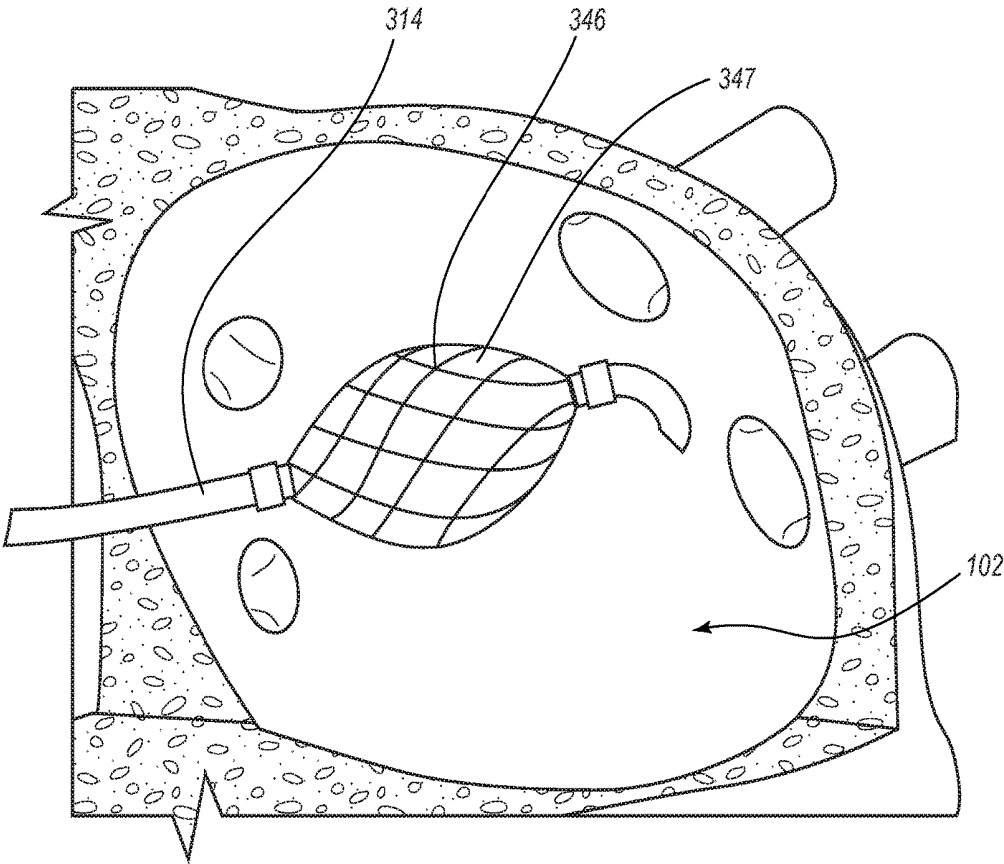


FIG. 18

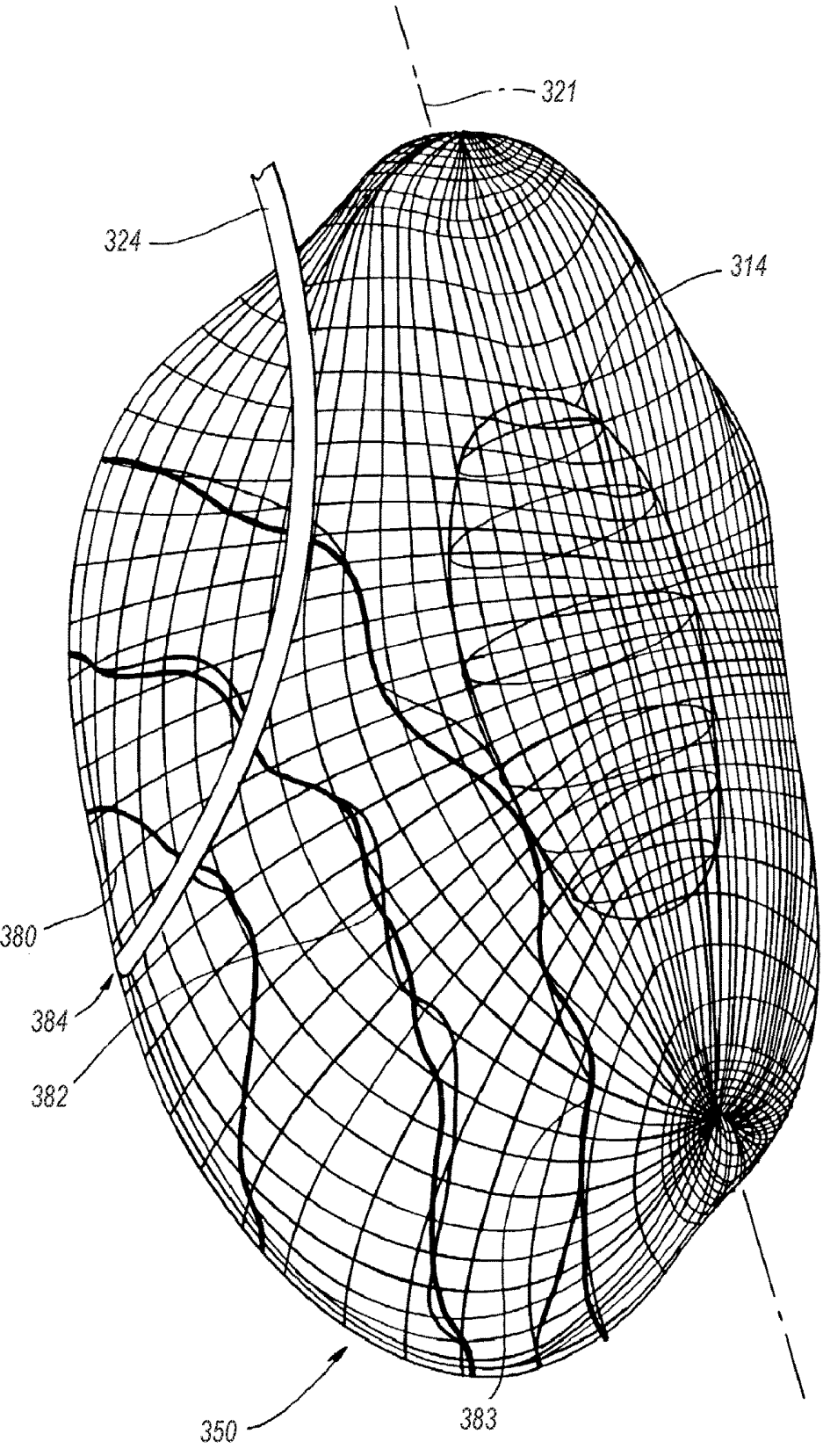


FIG. 19

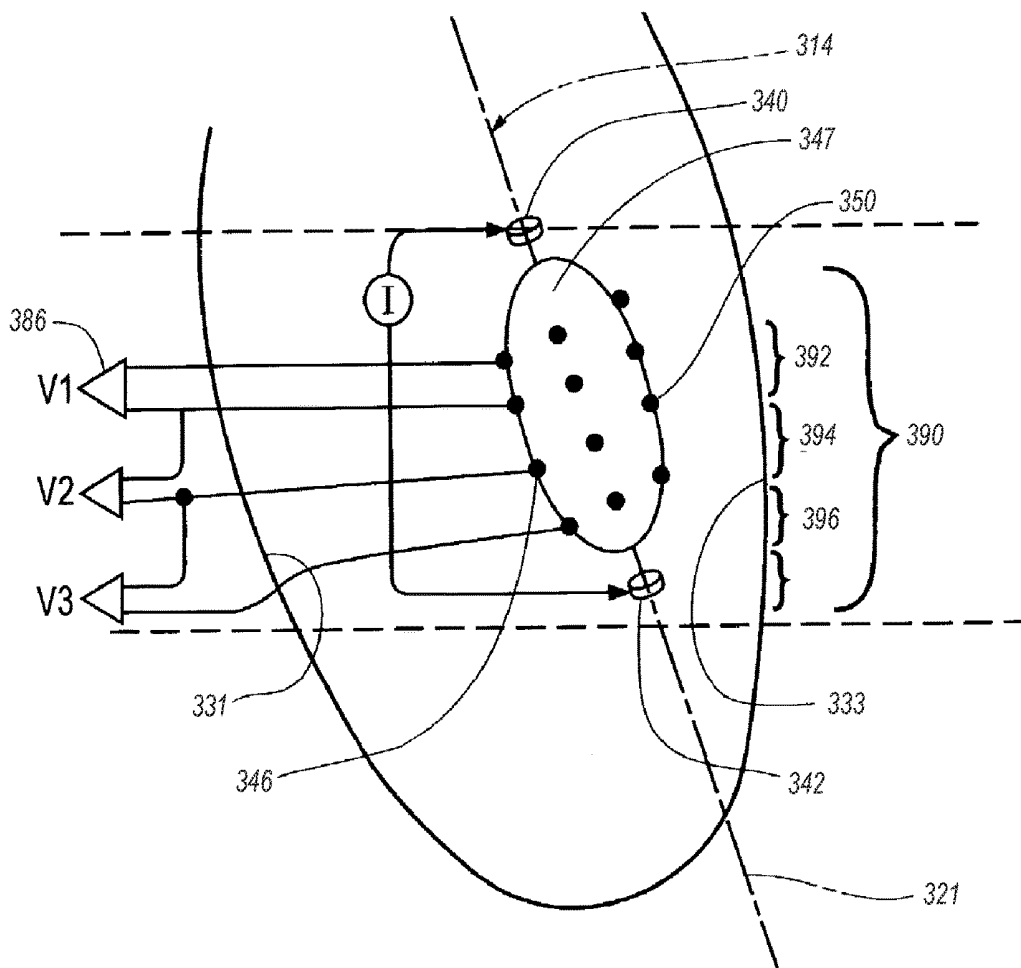
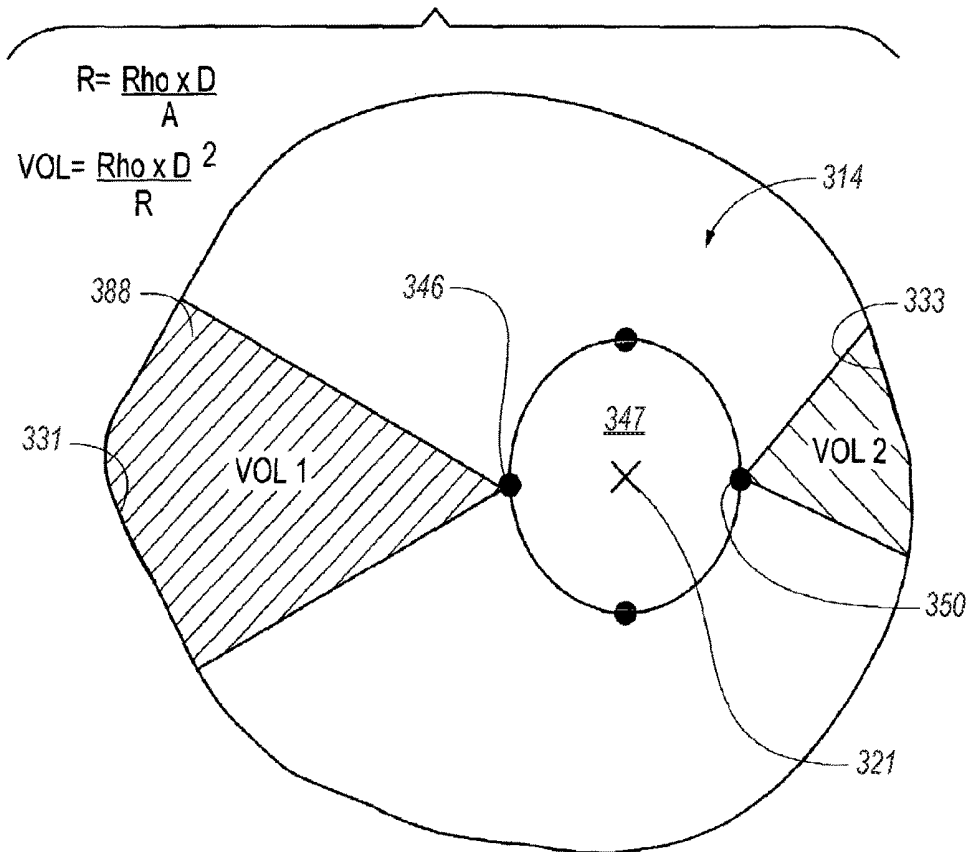


FIG. 20

FIG. 21



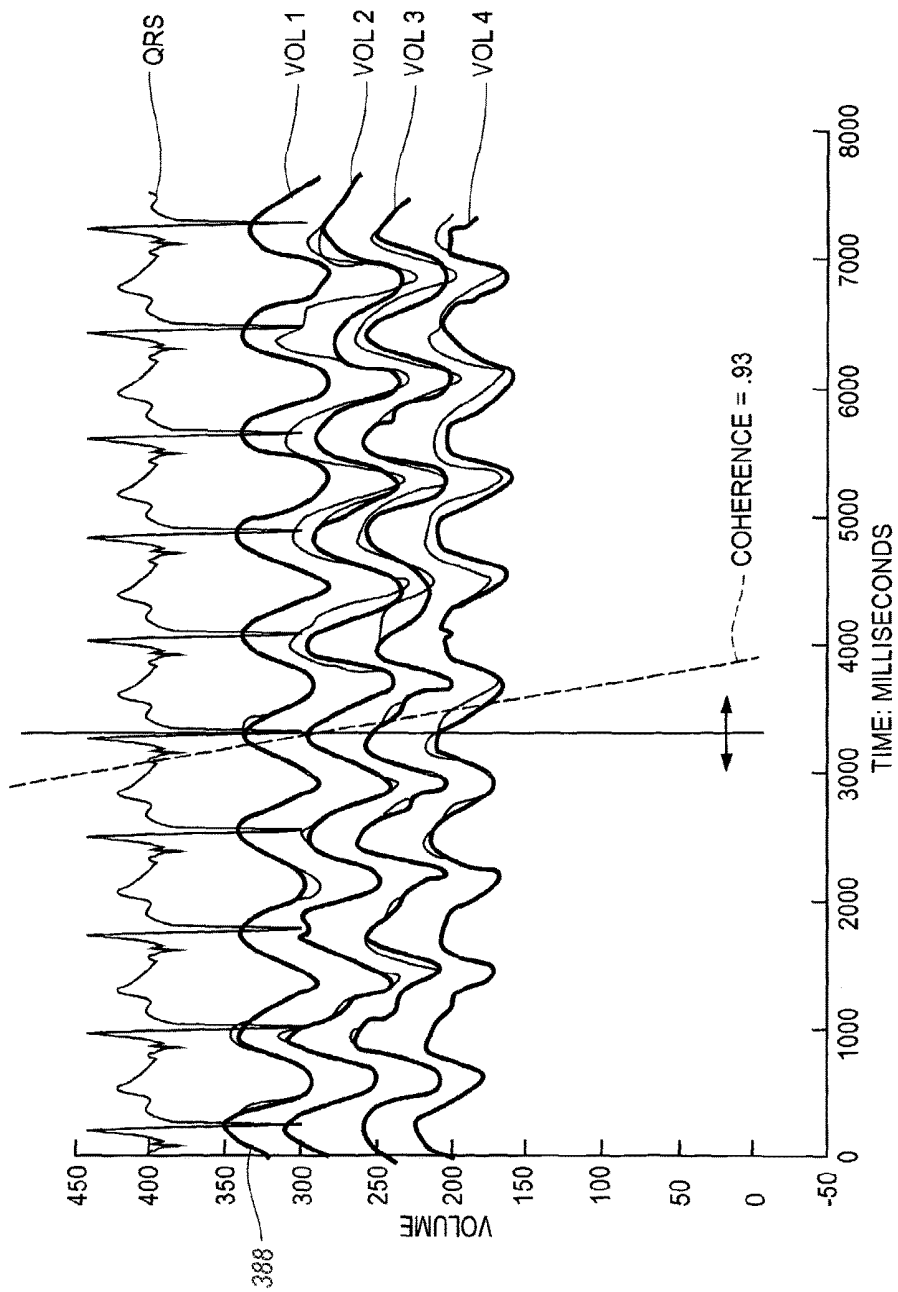


FIG. 22

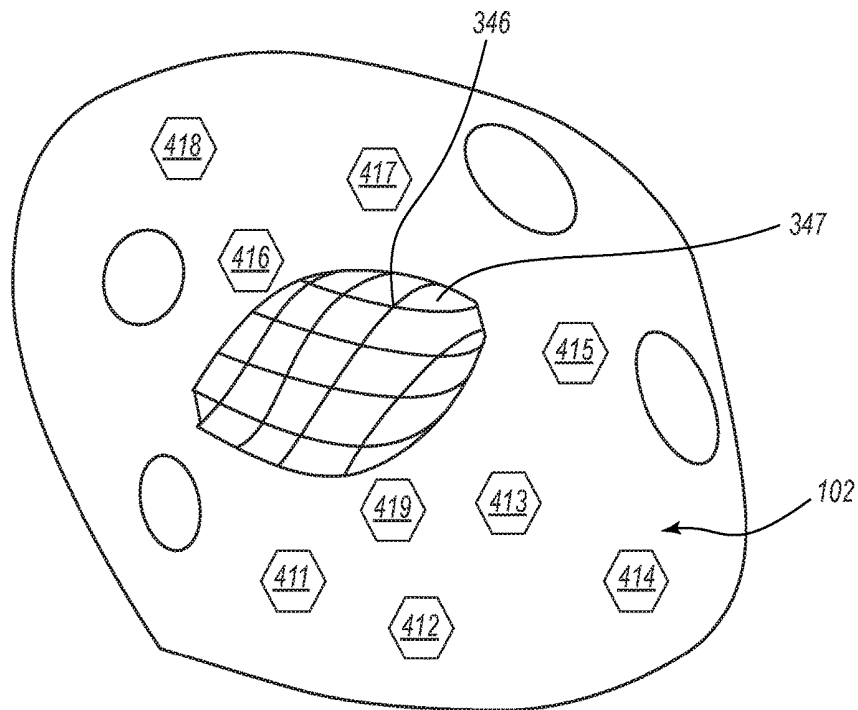


FIG. 23

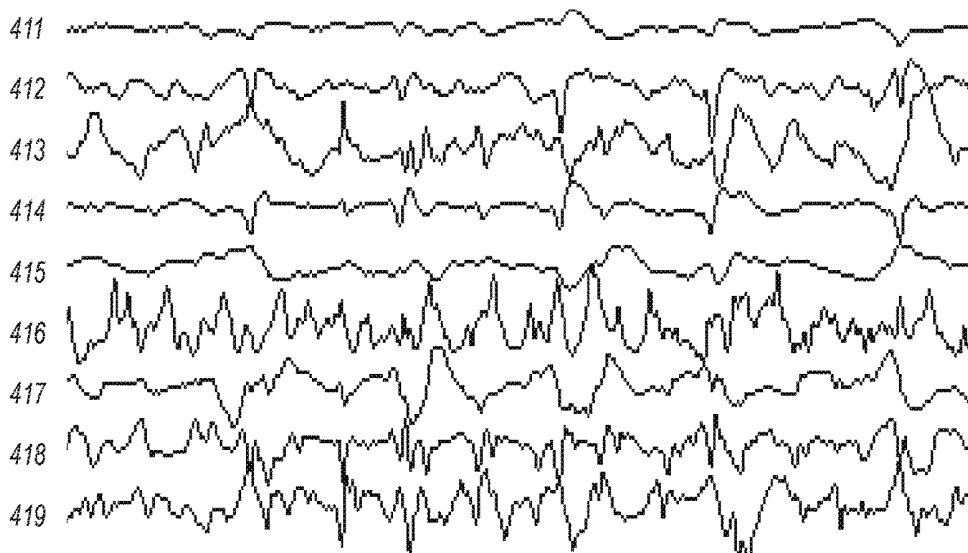


FIG. 24

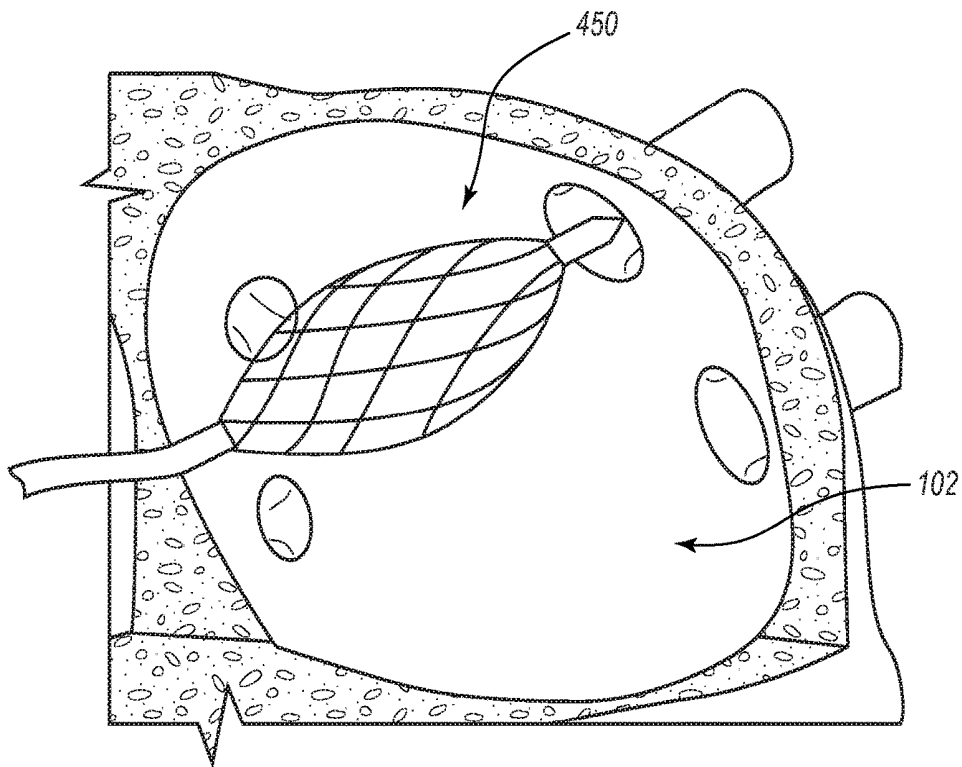


FIG. 25A

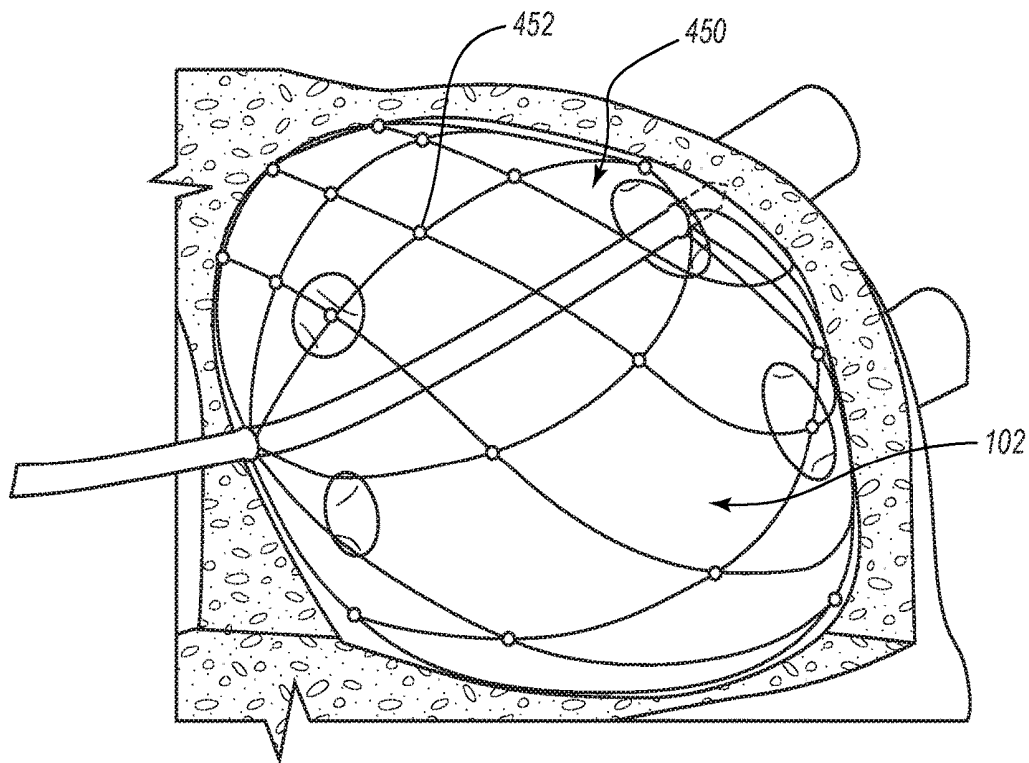


FIG. 25B

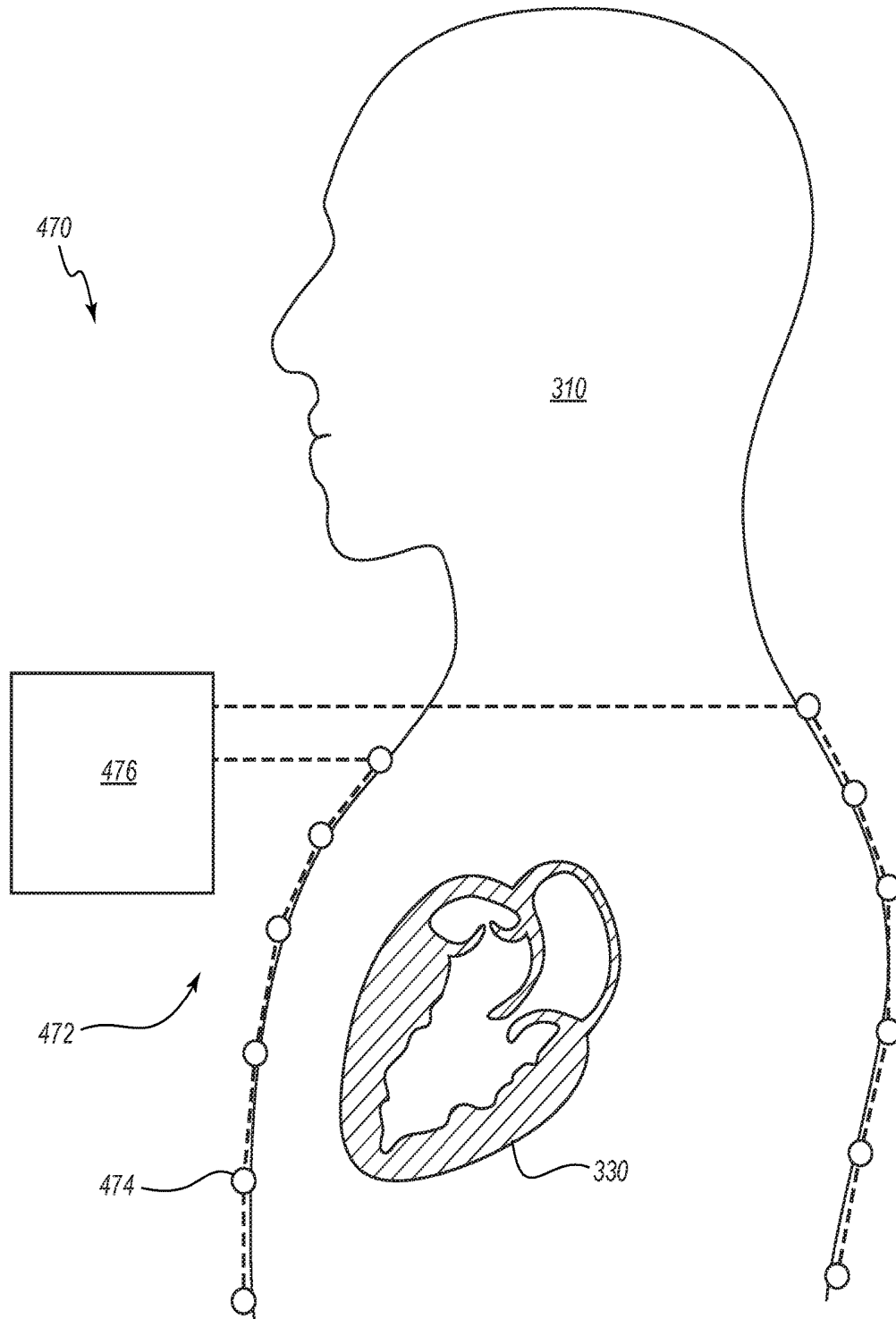
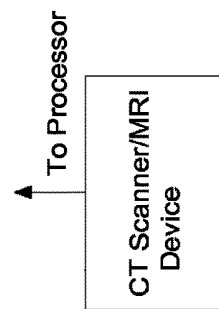
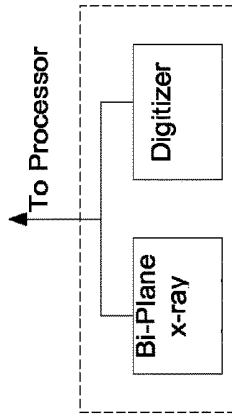
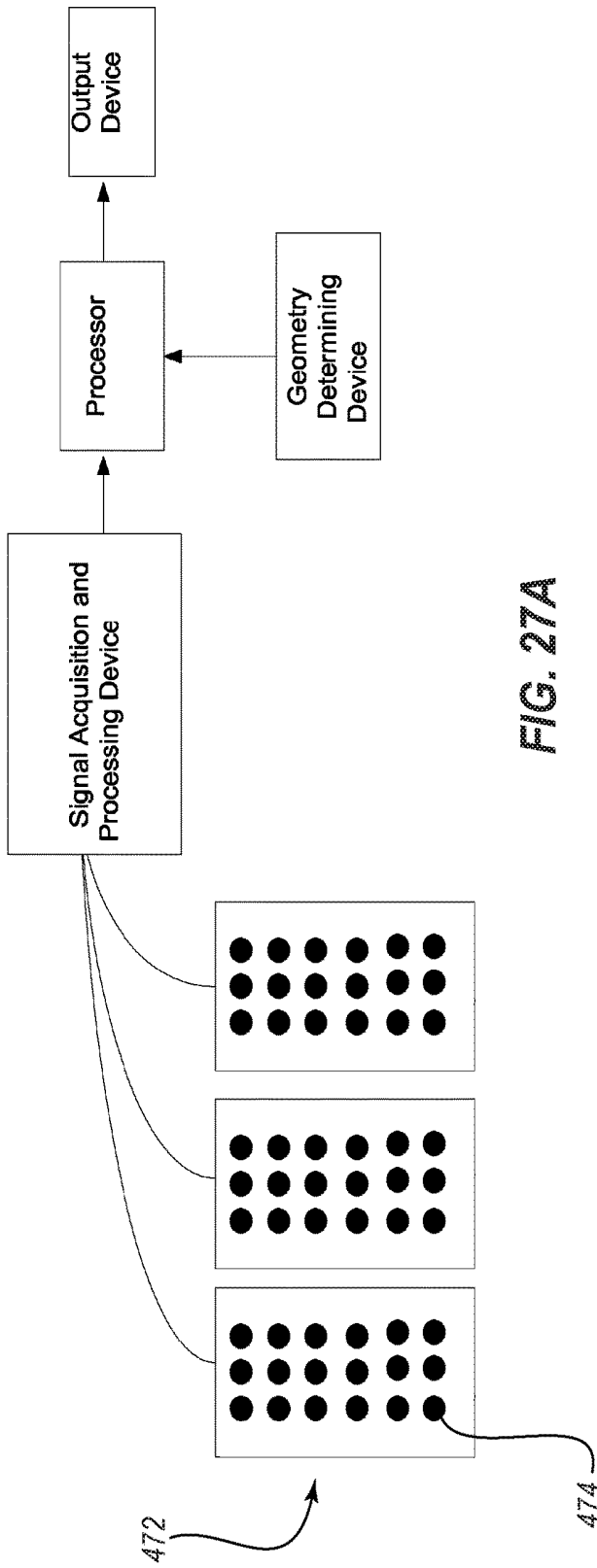


FIG. 26



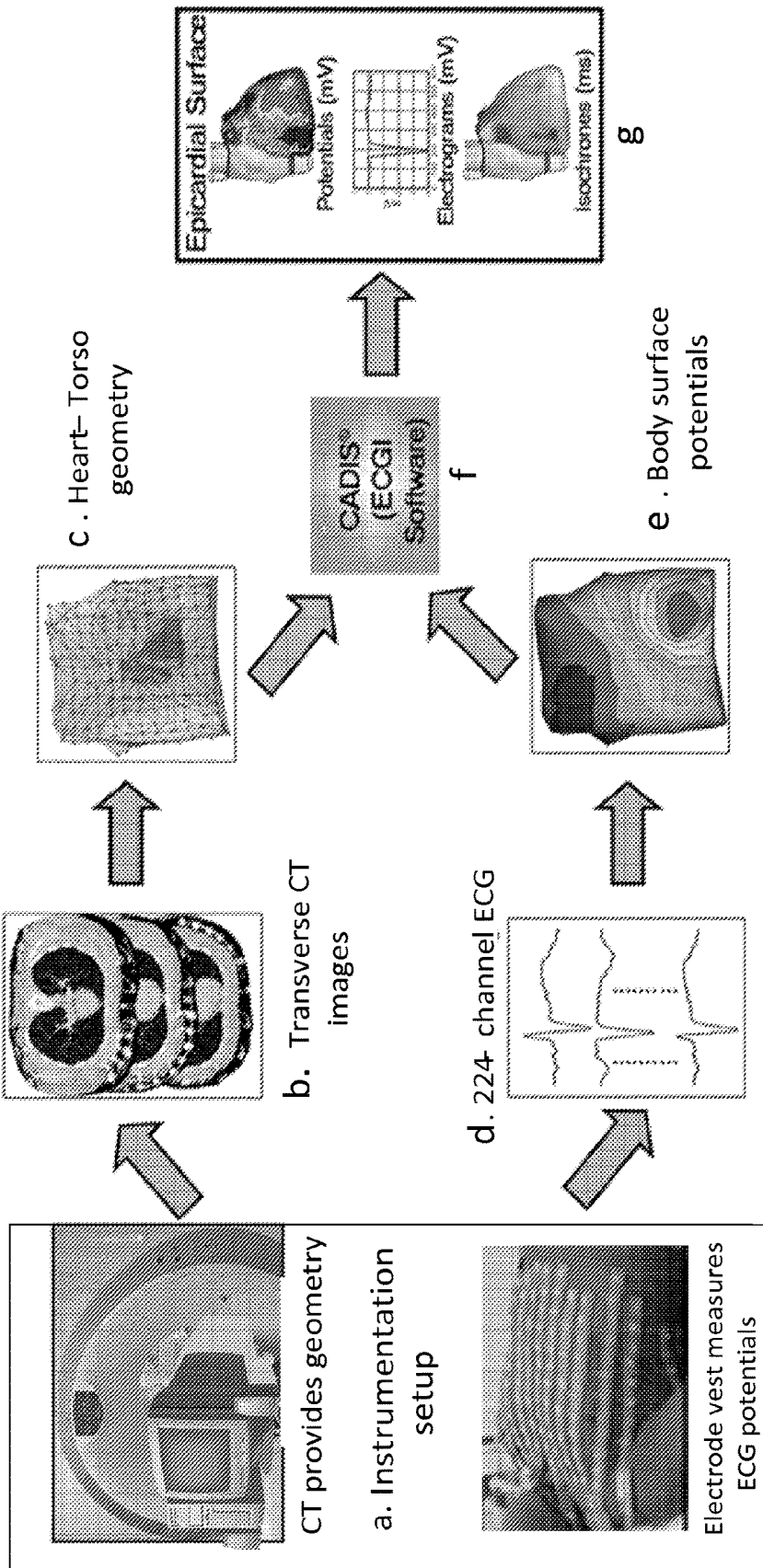


FIG. 27D

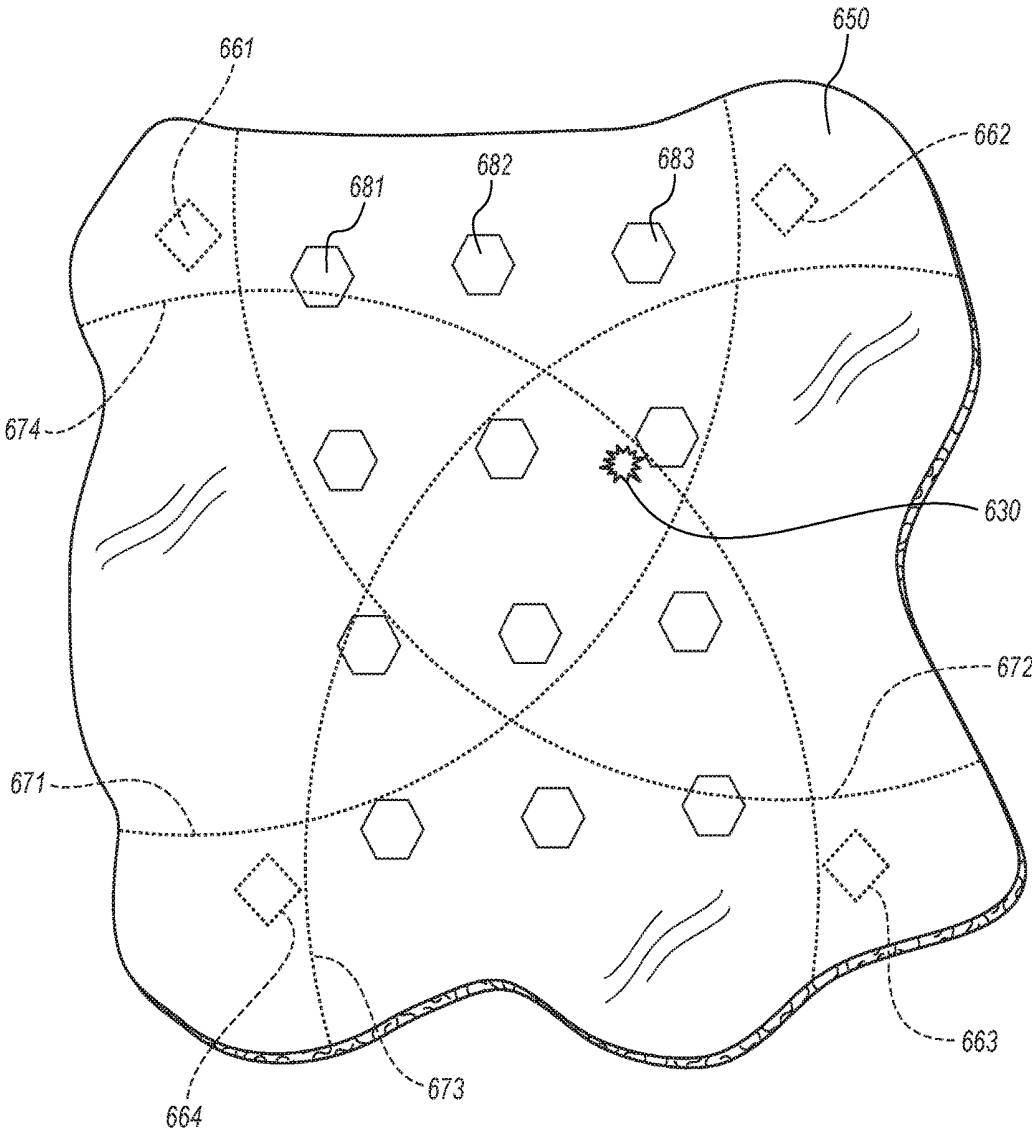
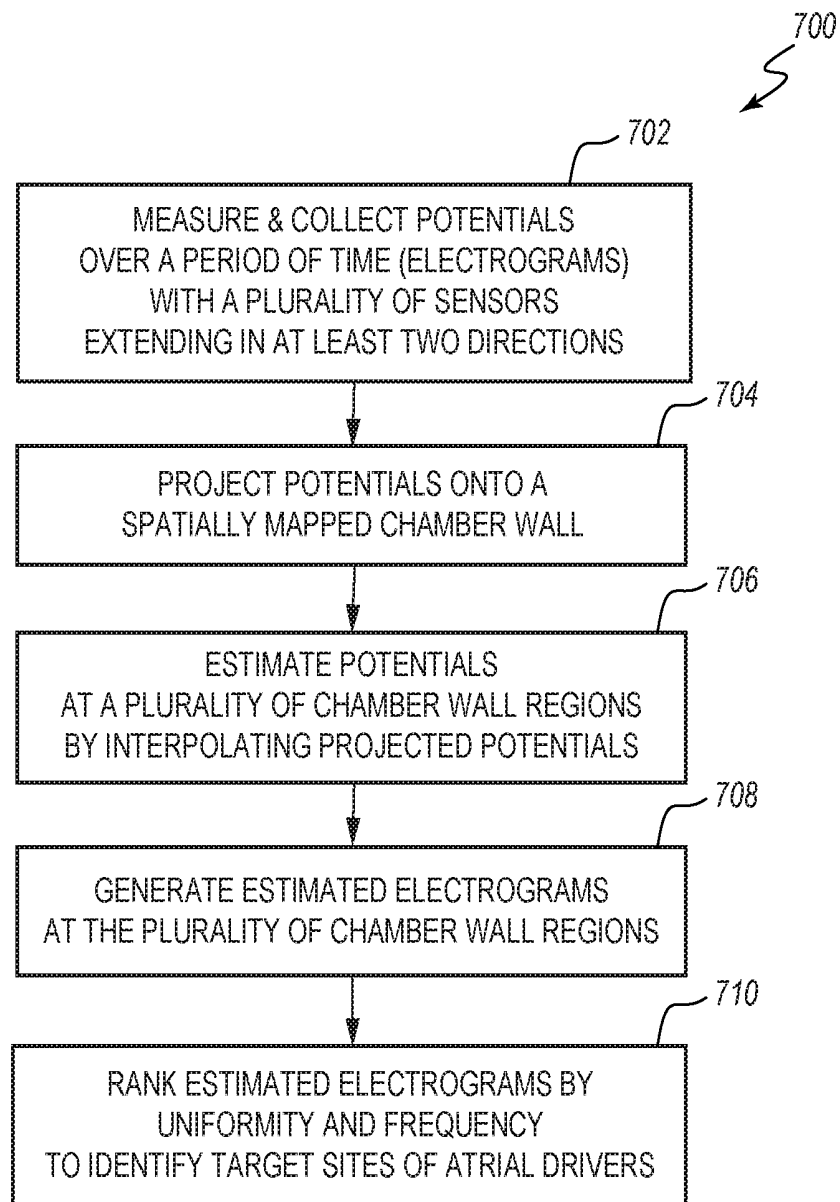


FIG. 28

**FIG. 29**

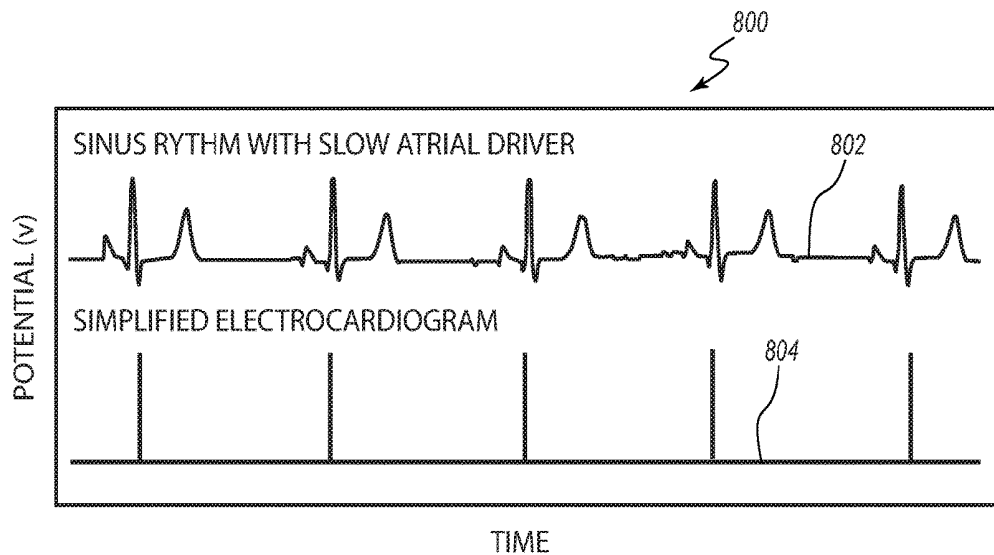


FIG. 30

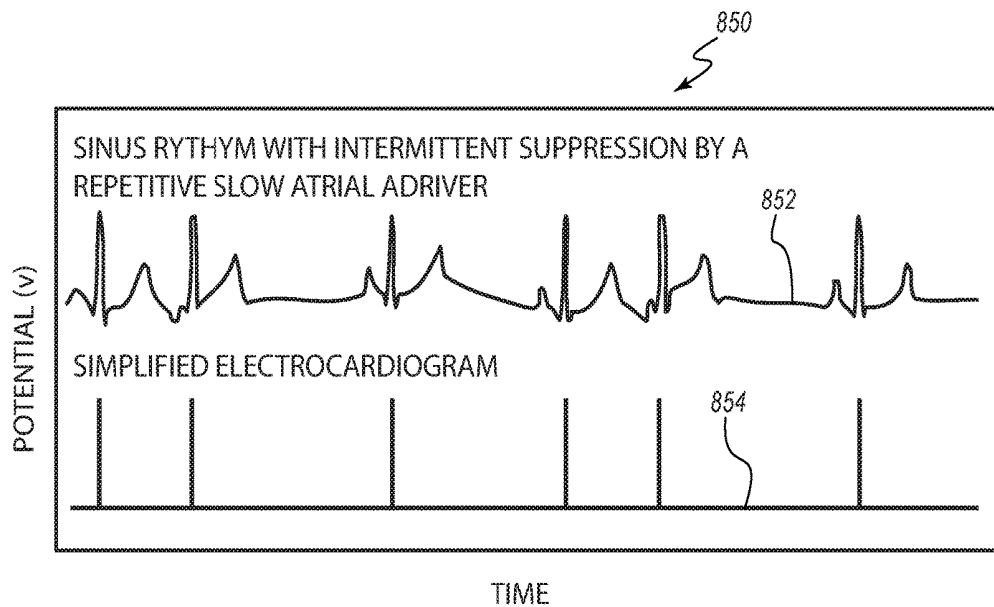


FIG. 31

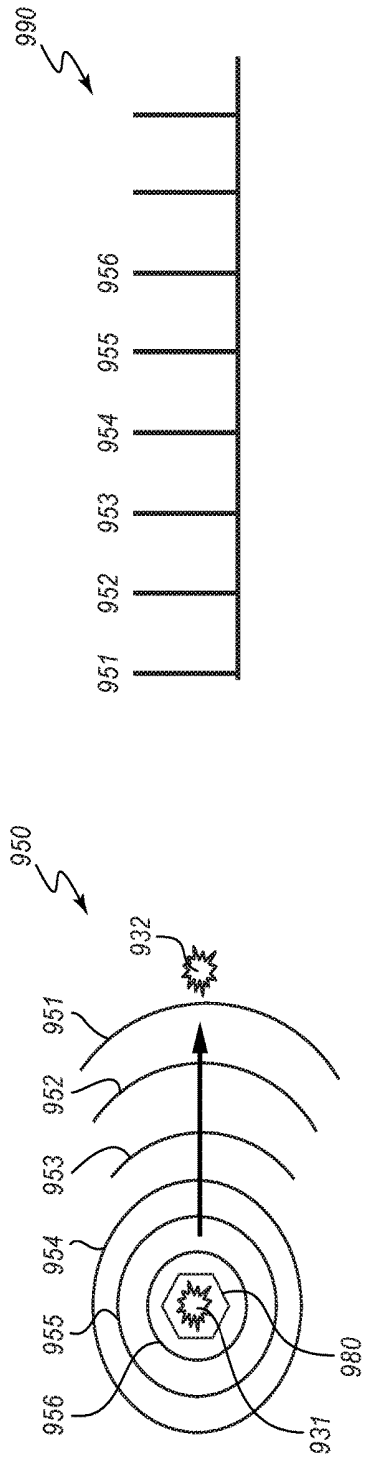


FIG. 32B

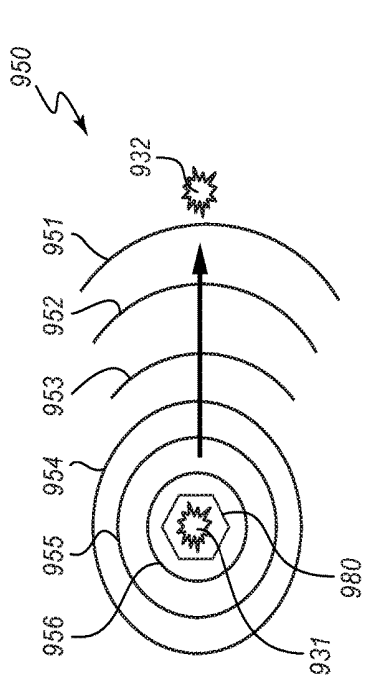


FIG. 32A

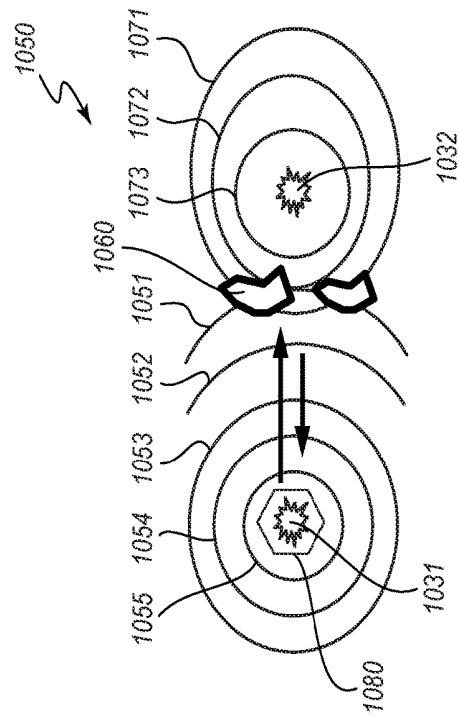


FIG. 33A

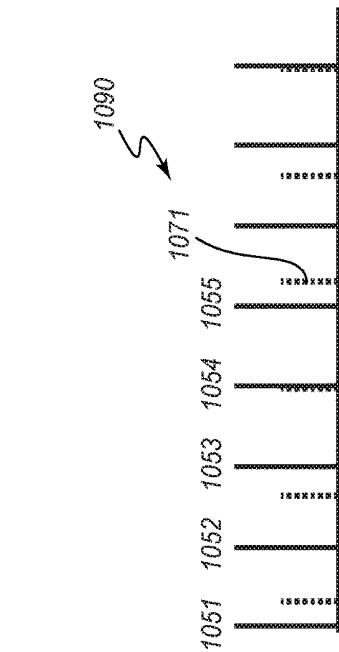


FIG. 33B

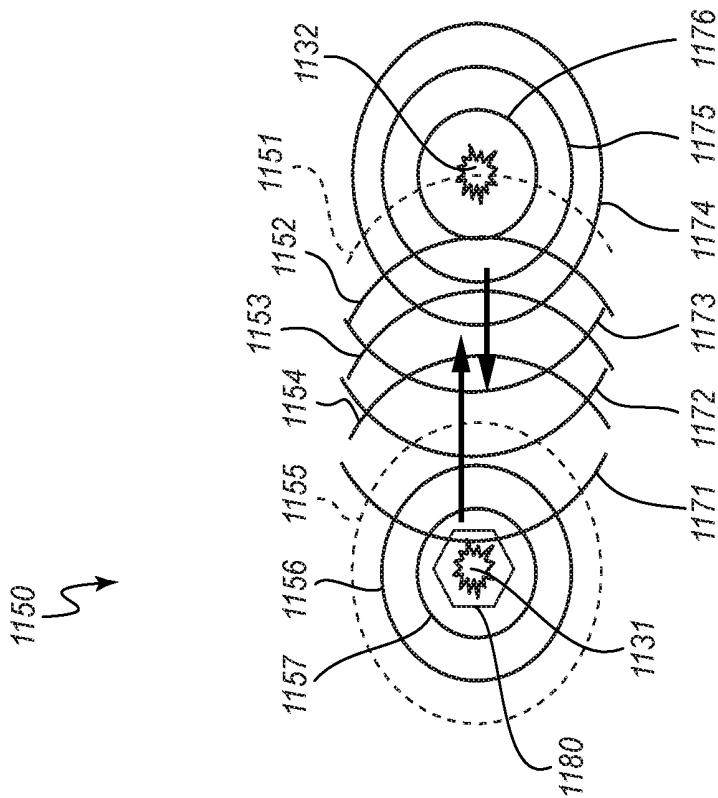


FIG. 34A

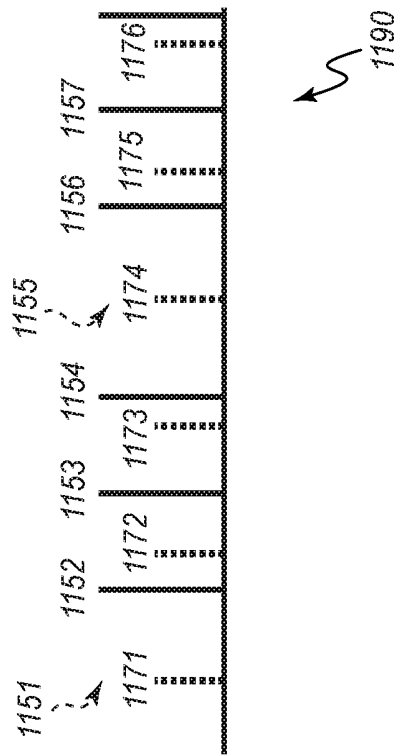


FIG. 34B

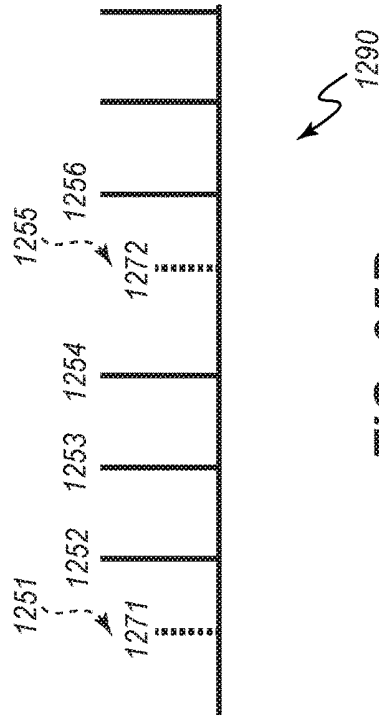
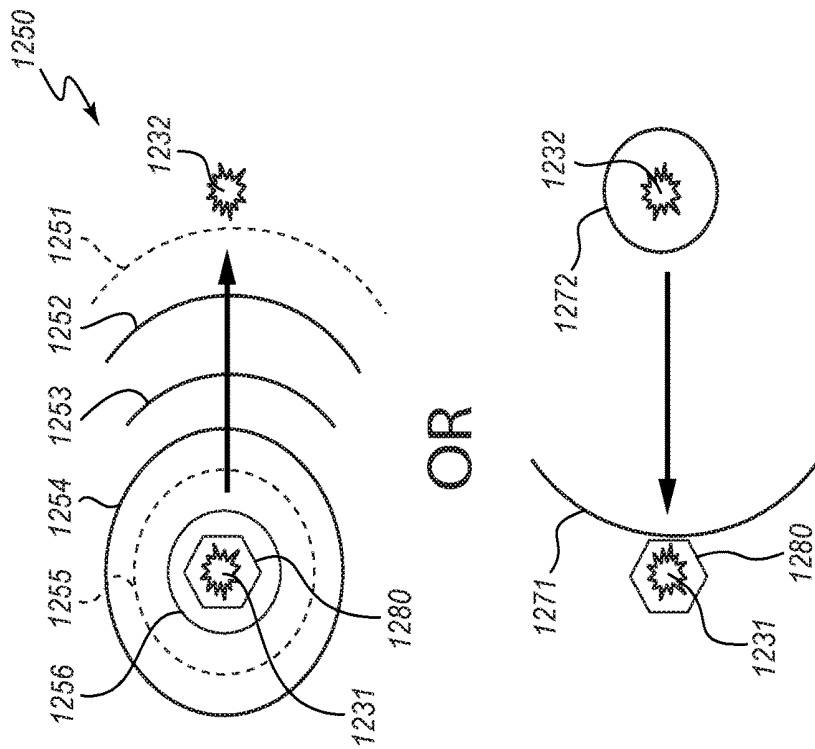


FIG. 35B

FIG. 35A

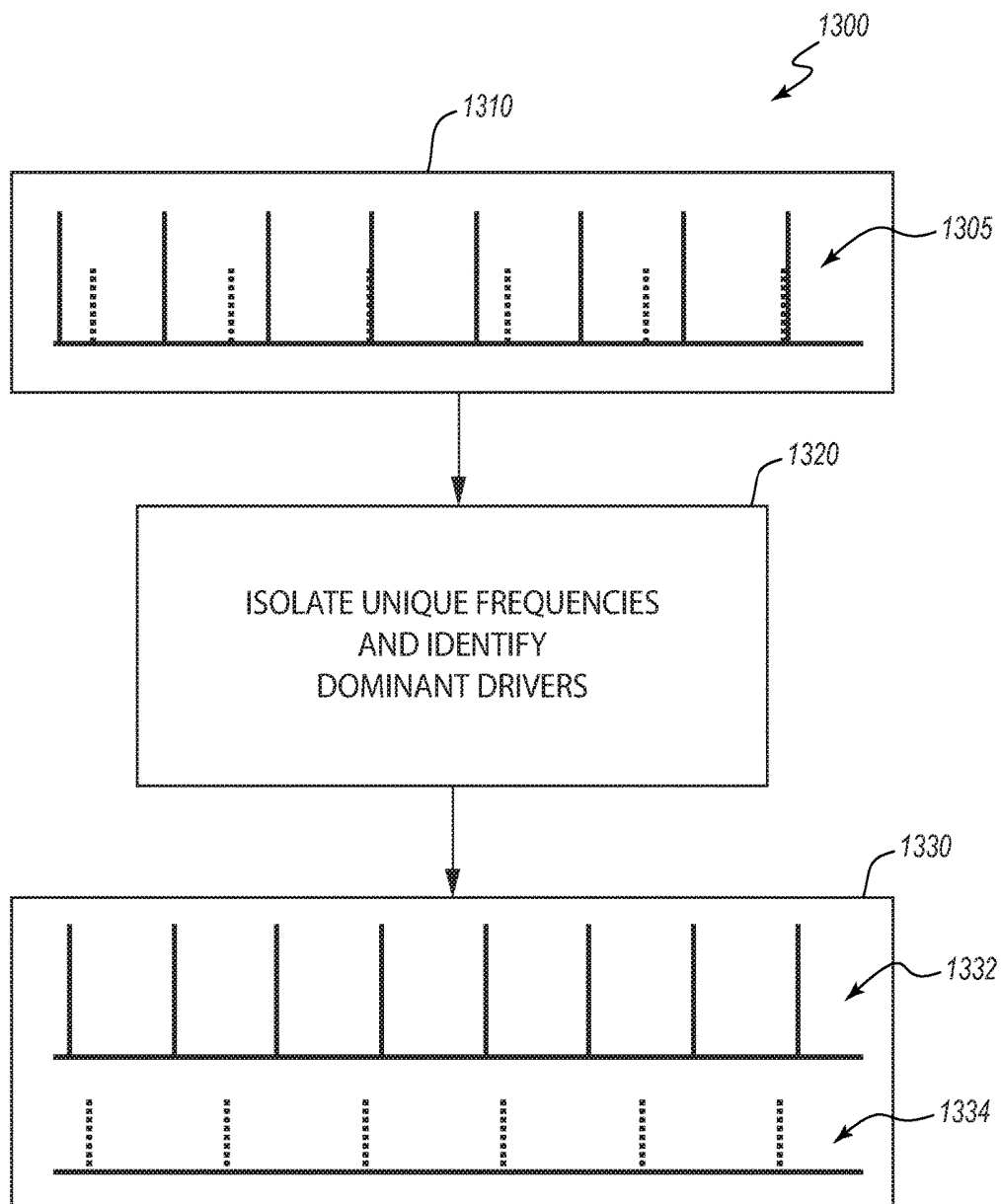


FIG. 36

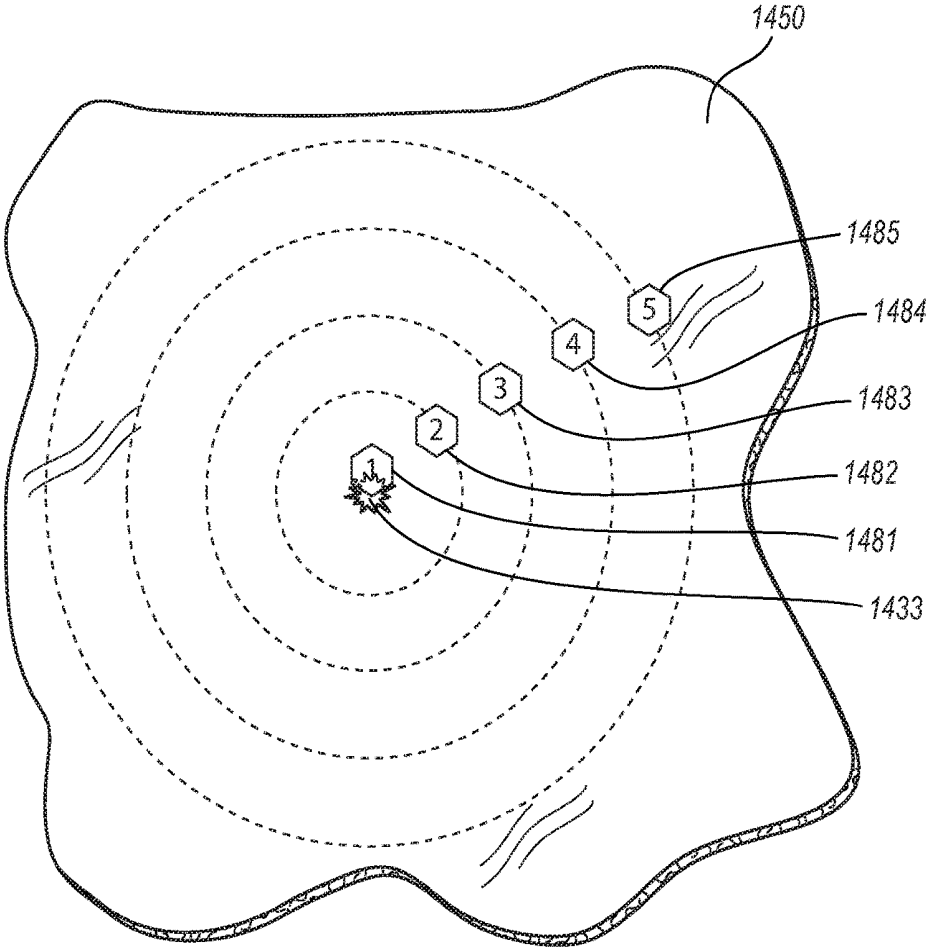


FIG. 37

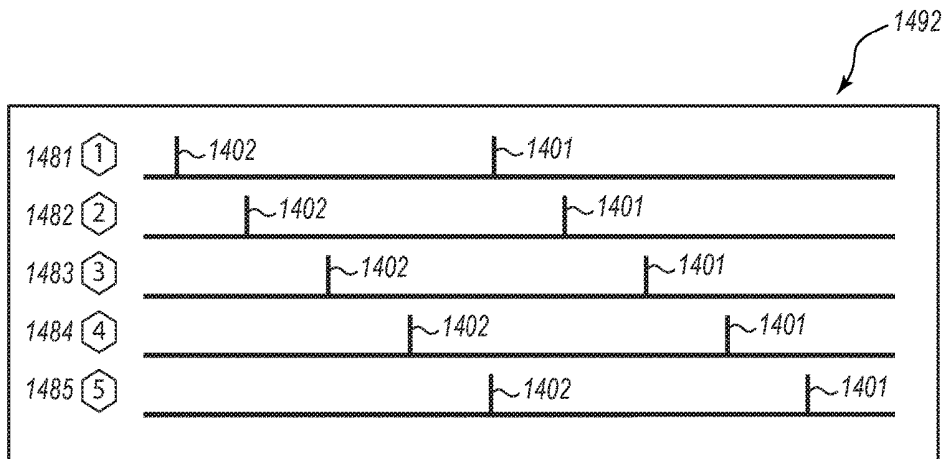


FIG. 38A

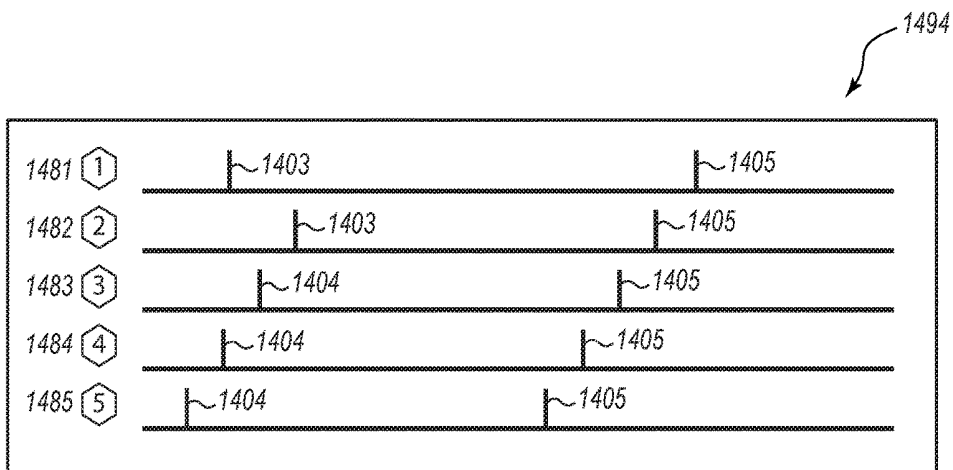


FIG. 38B

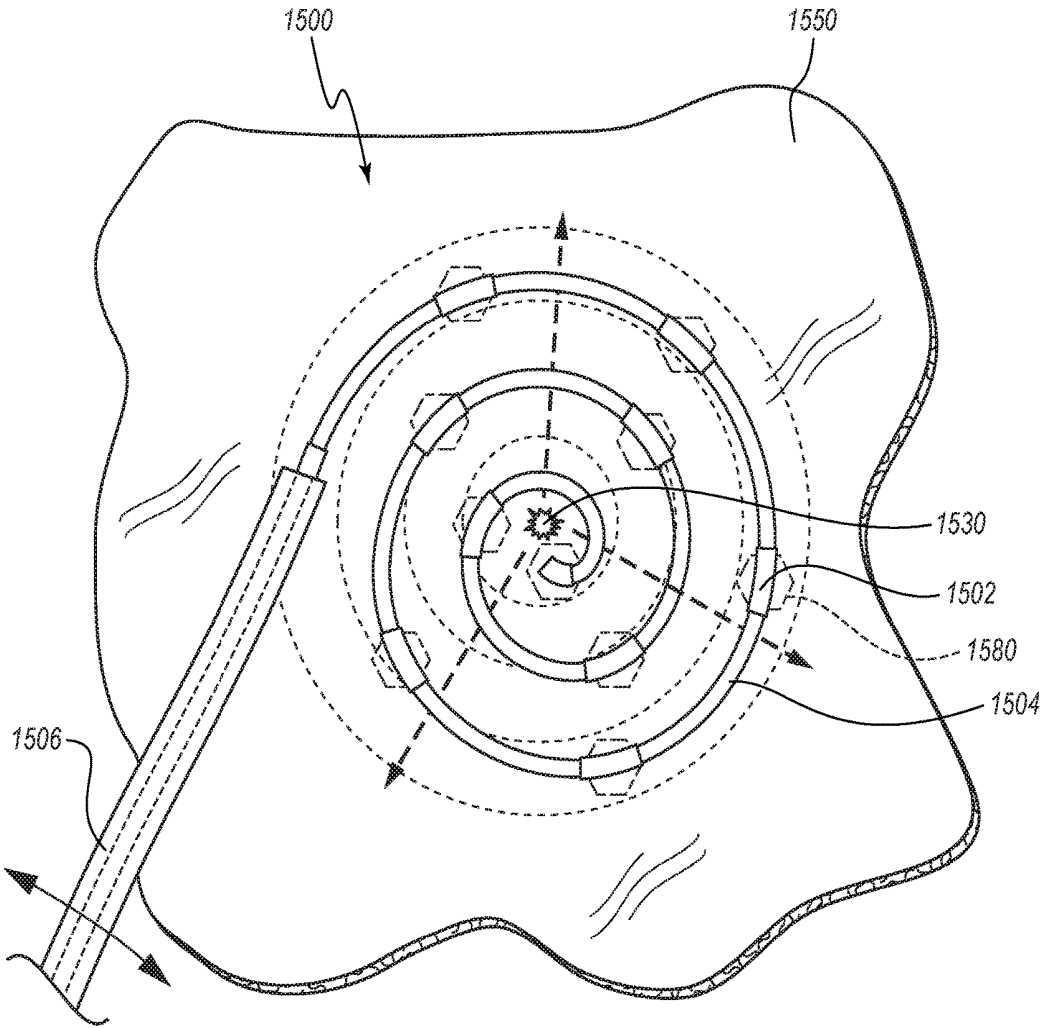


FIG. 39

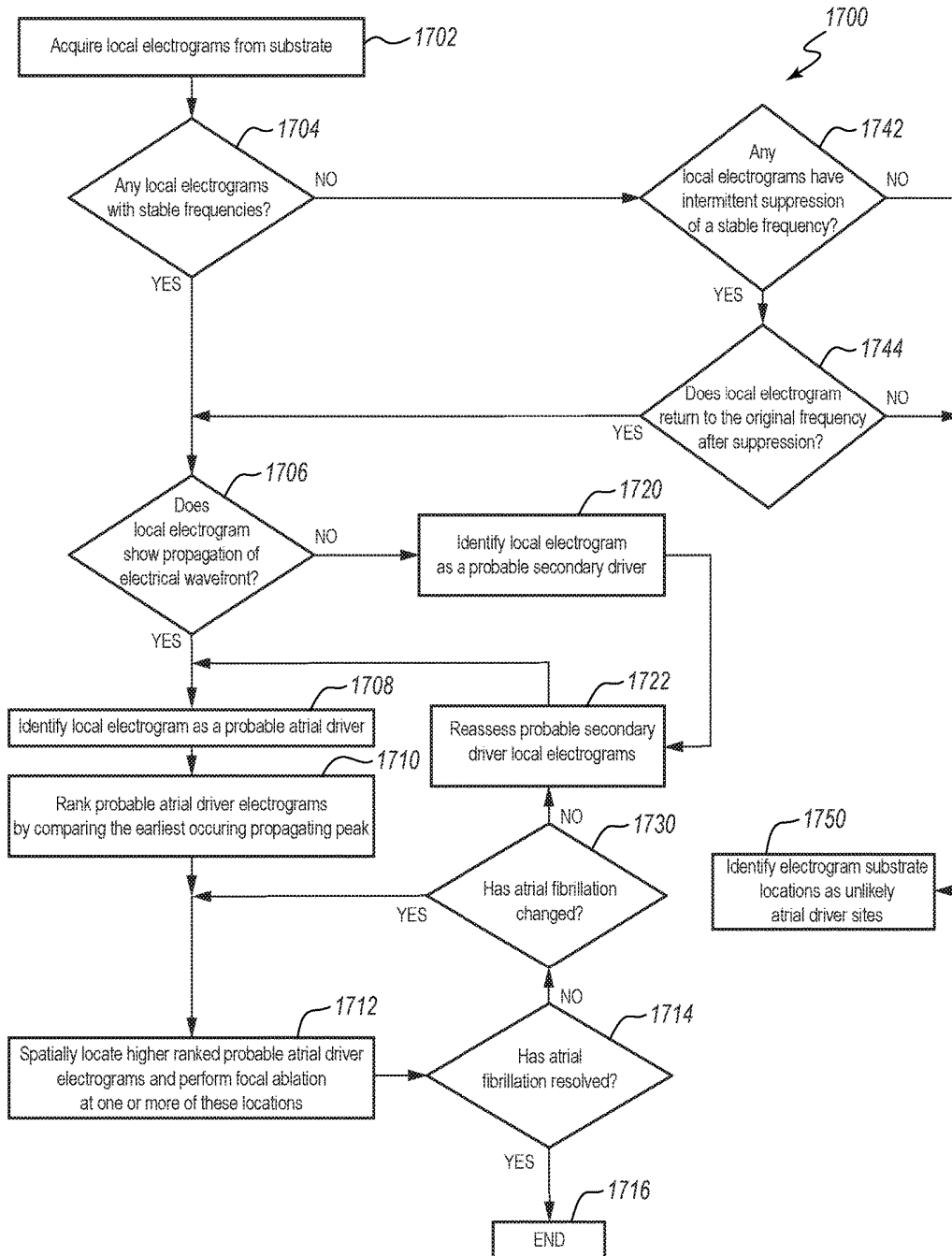


FIG. 41

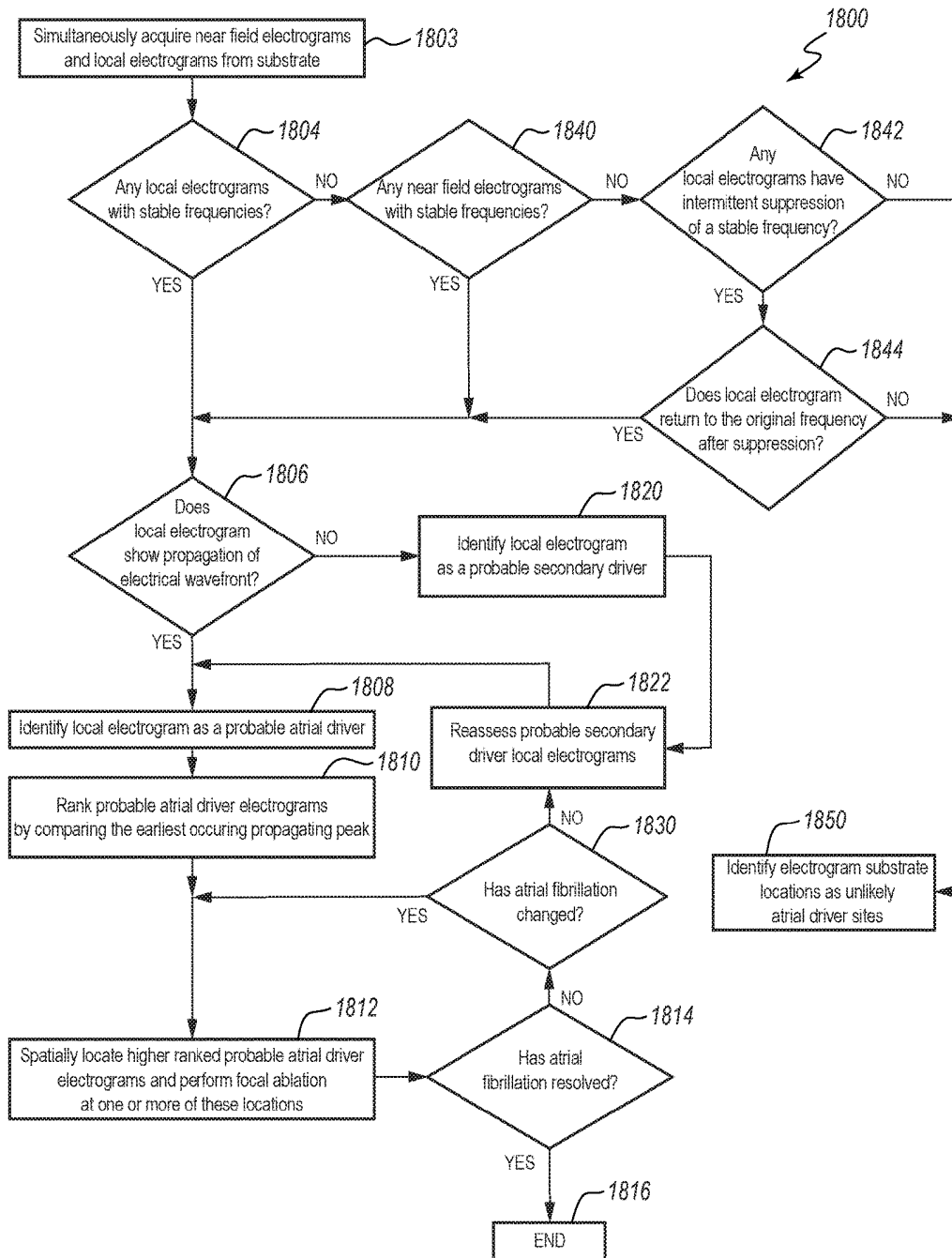


FIG. 42

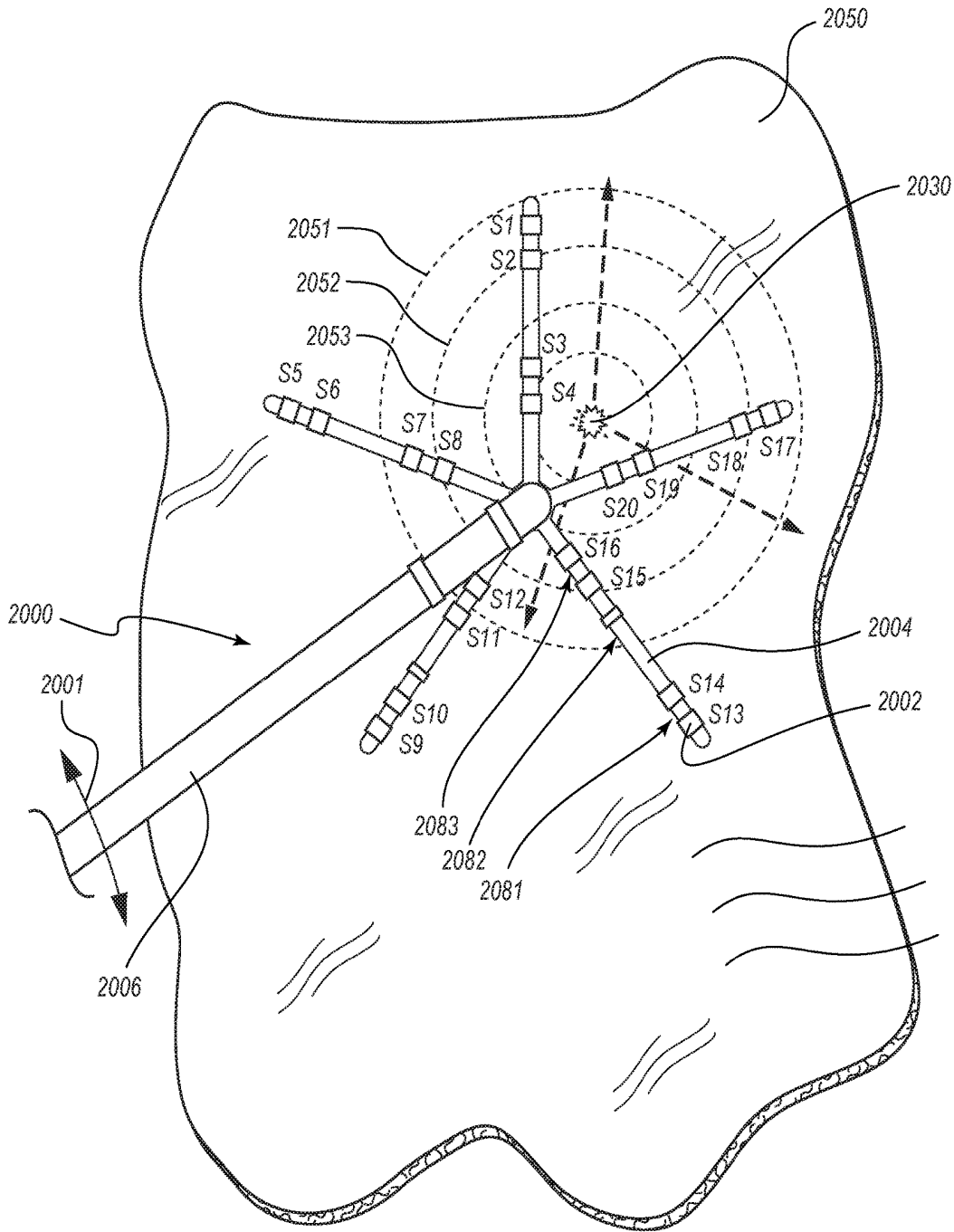


FIG. 43

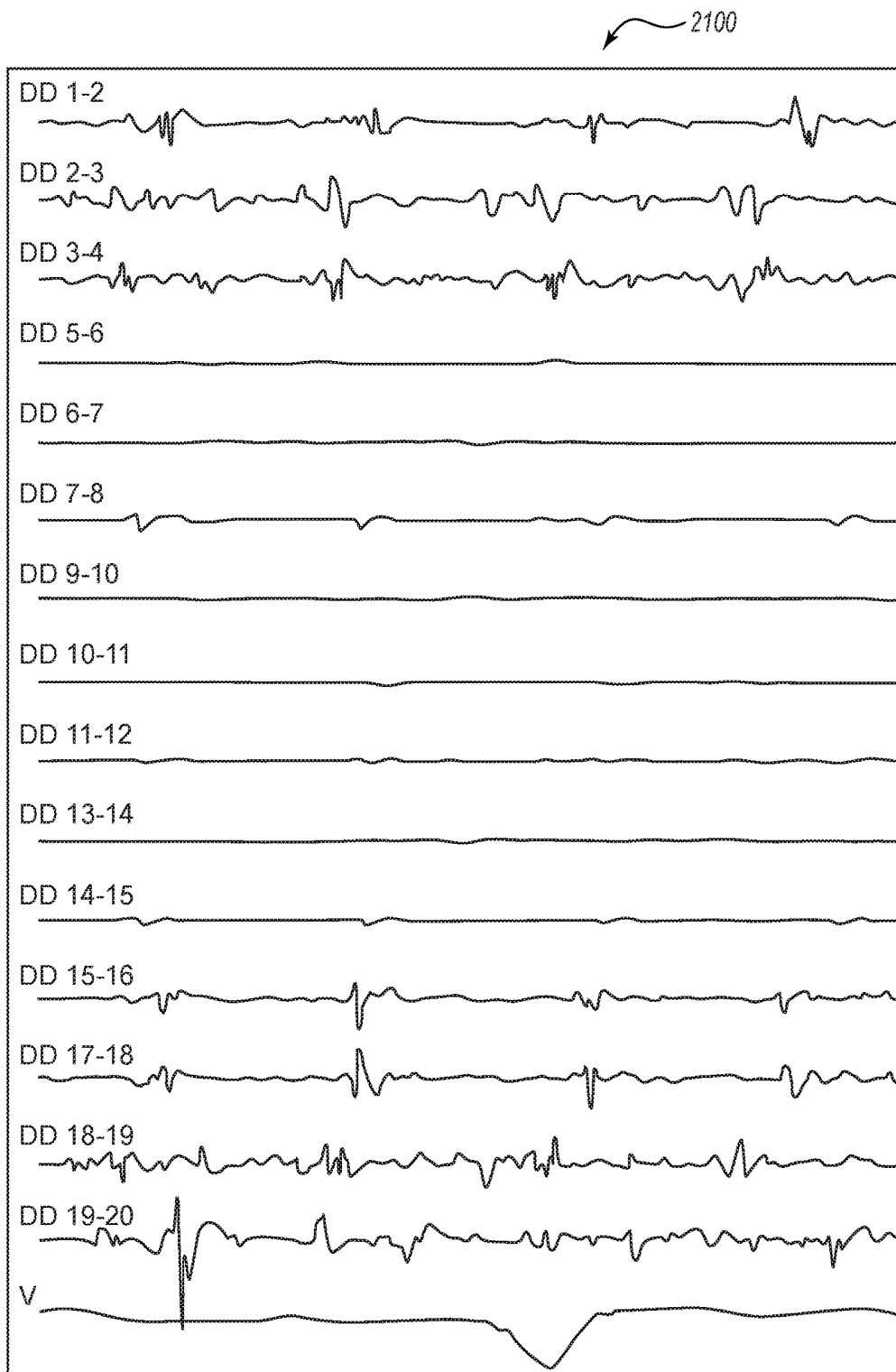


FIG. 44A

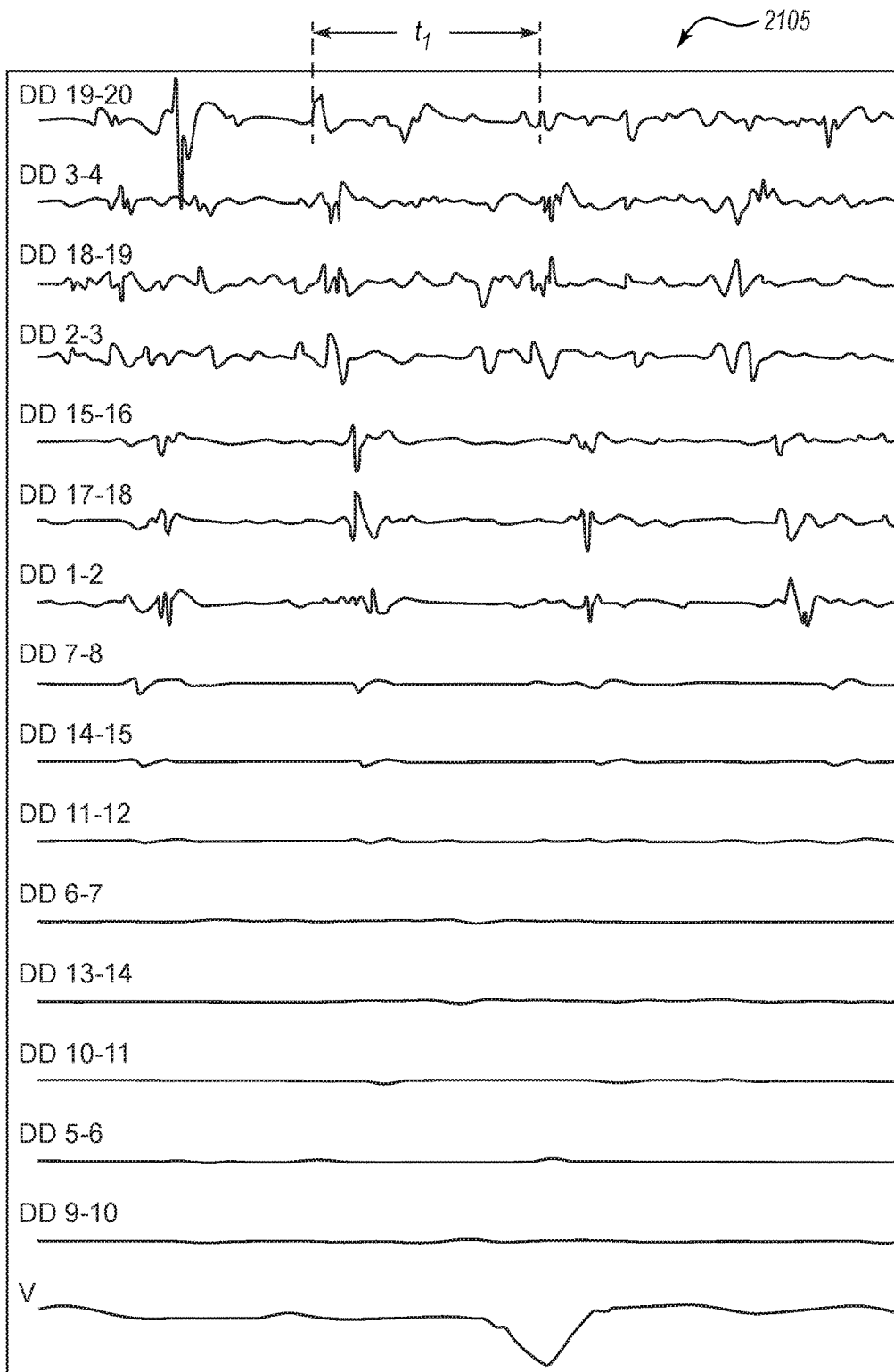


FIG. 44B

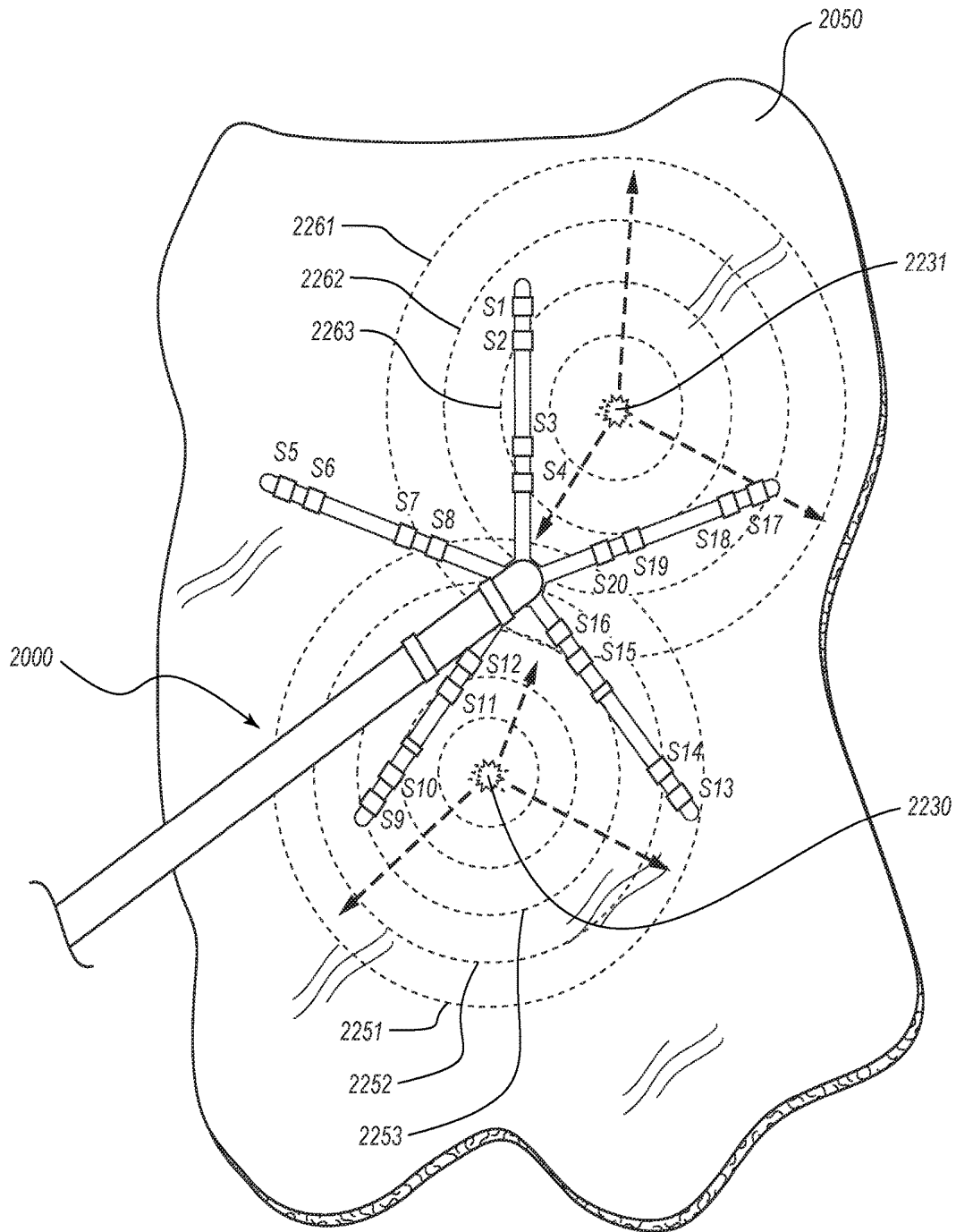


FIG. 45

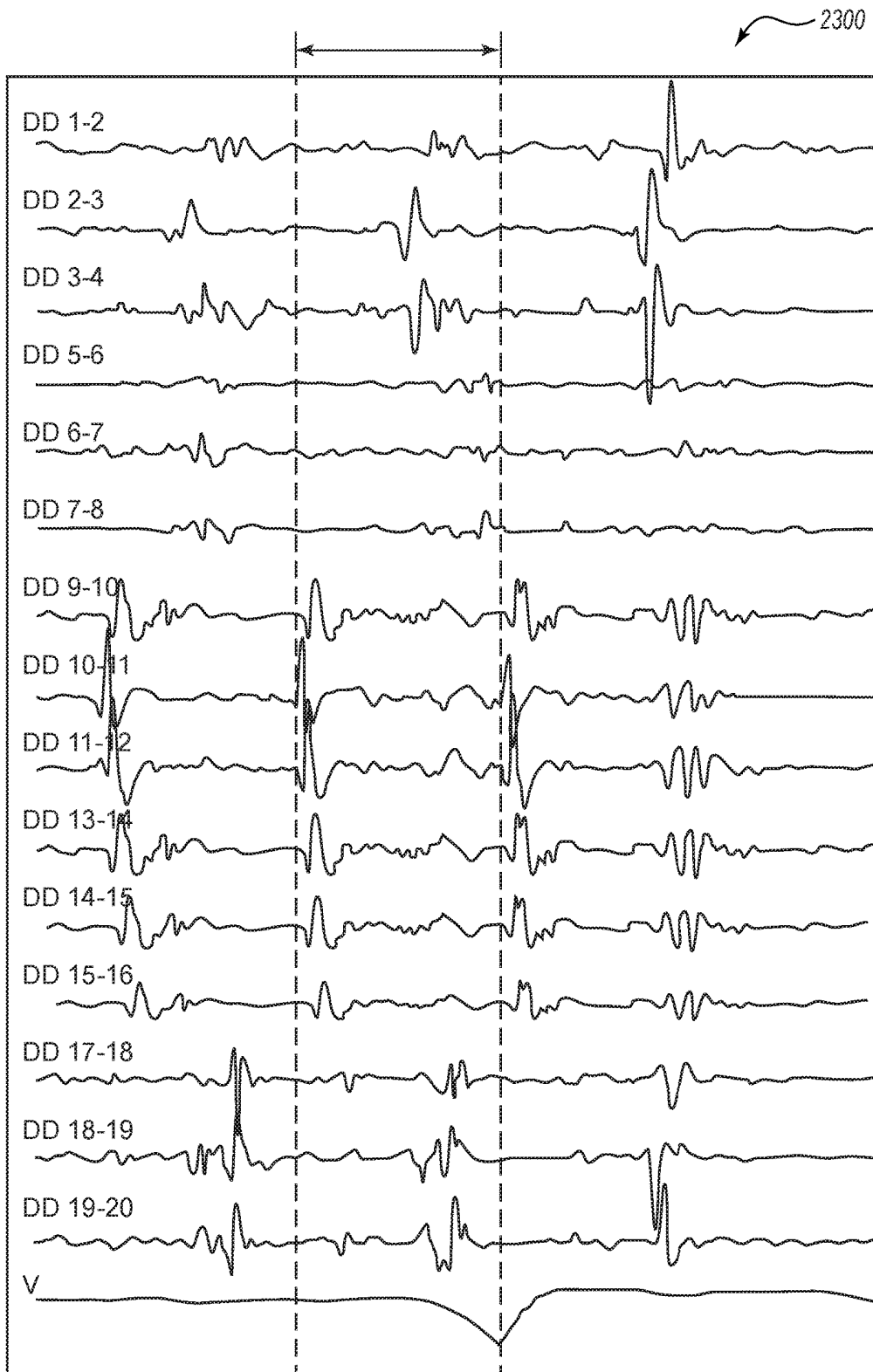


FIG. 46A

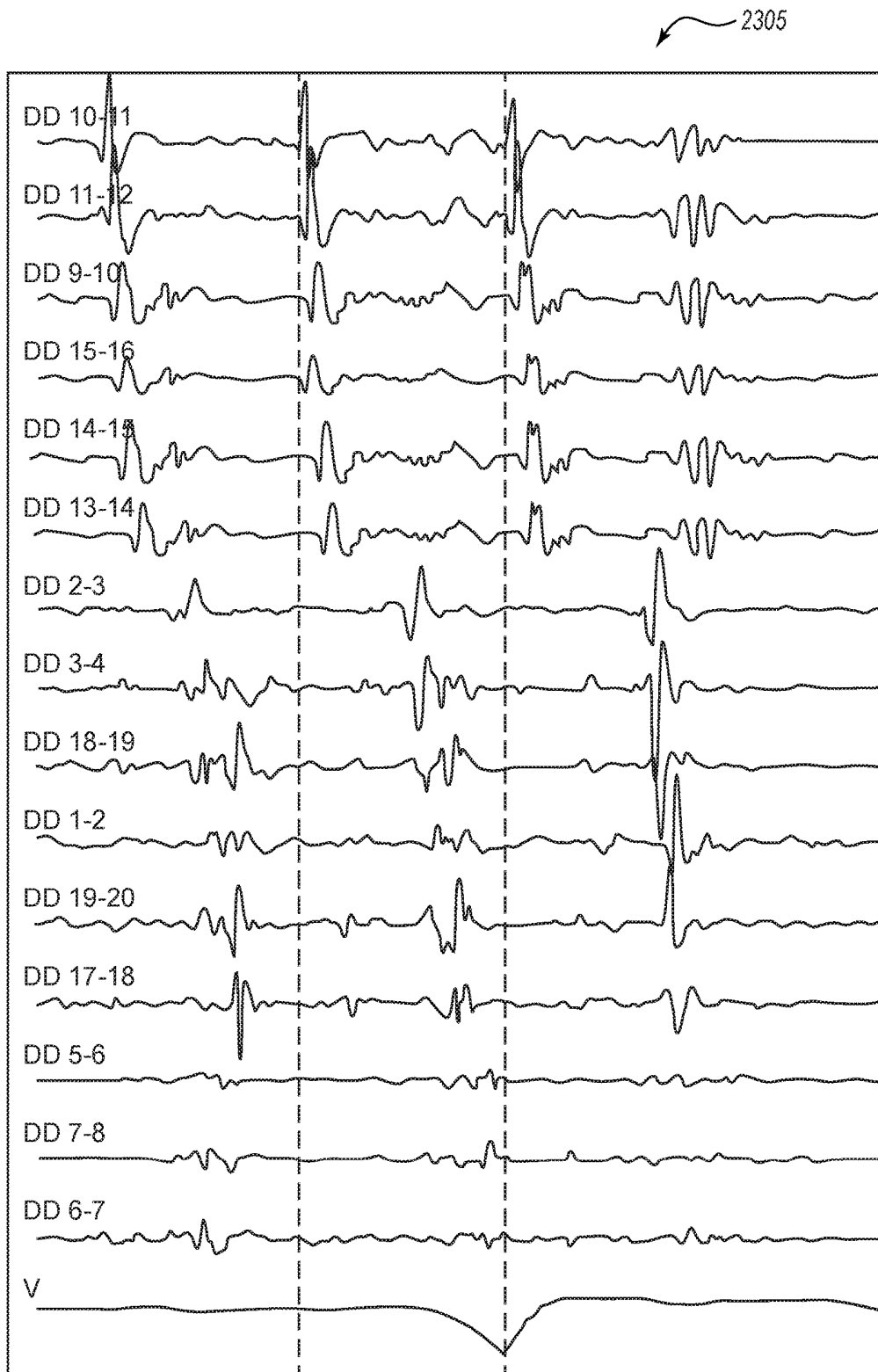


FIG. 46B

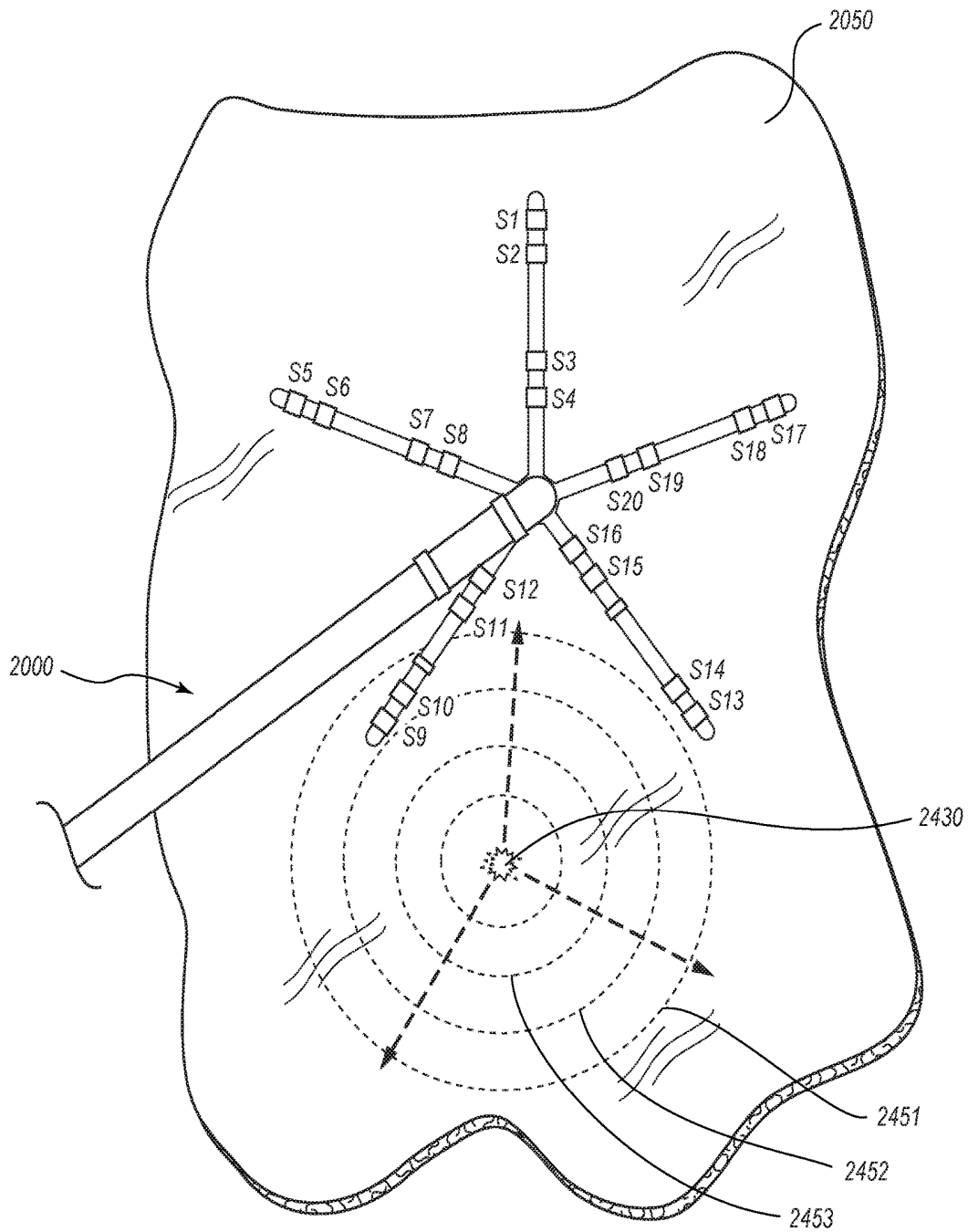


FIG. 47

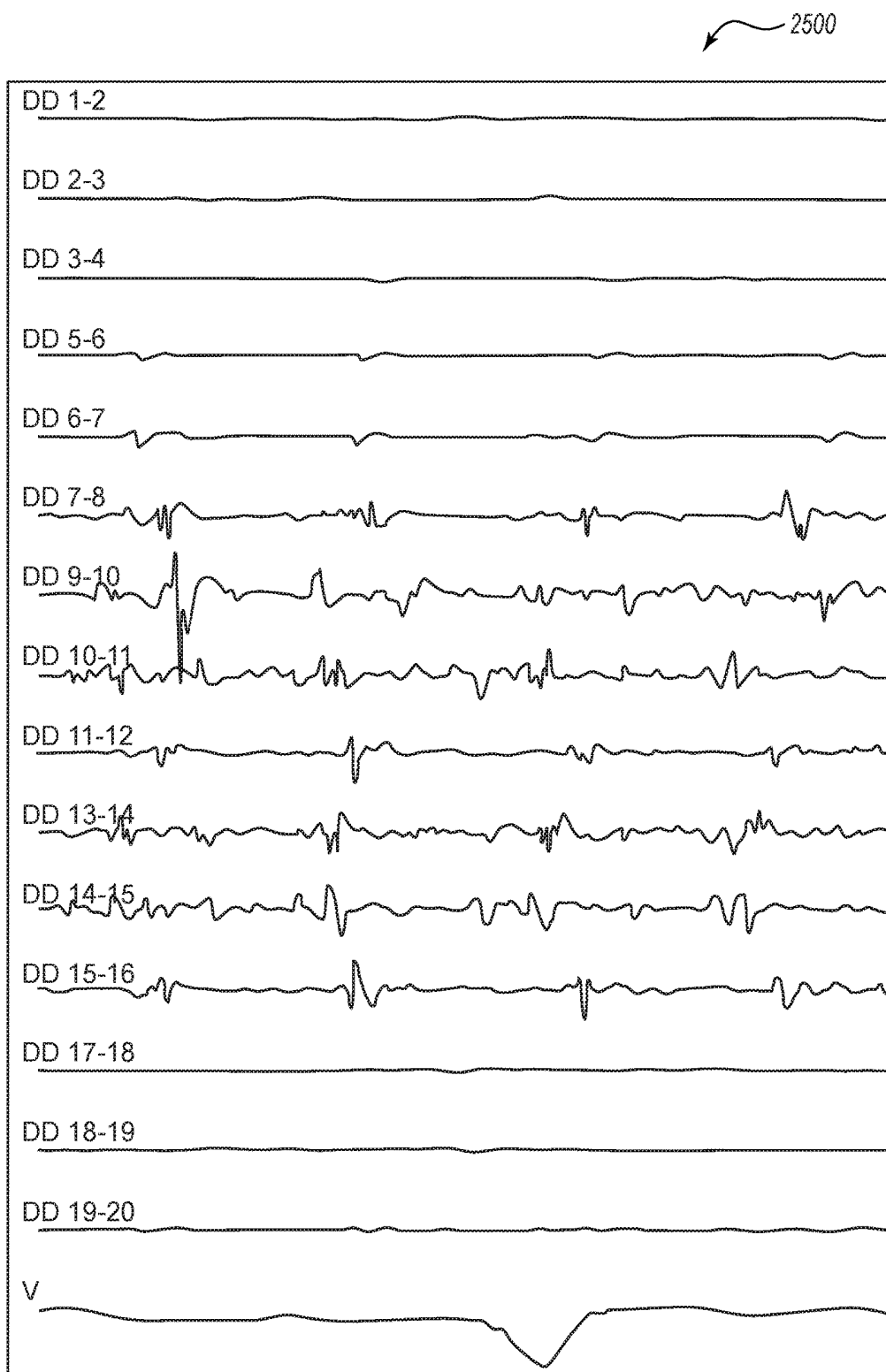


FIG. 48A

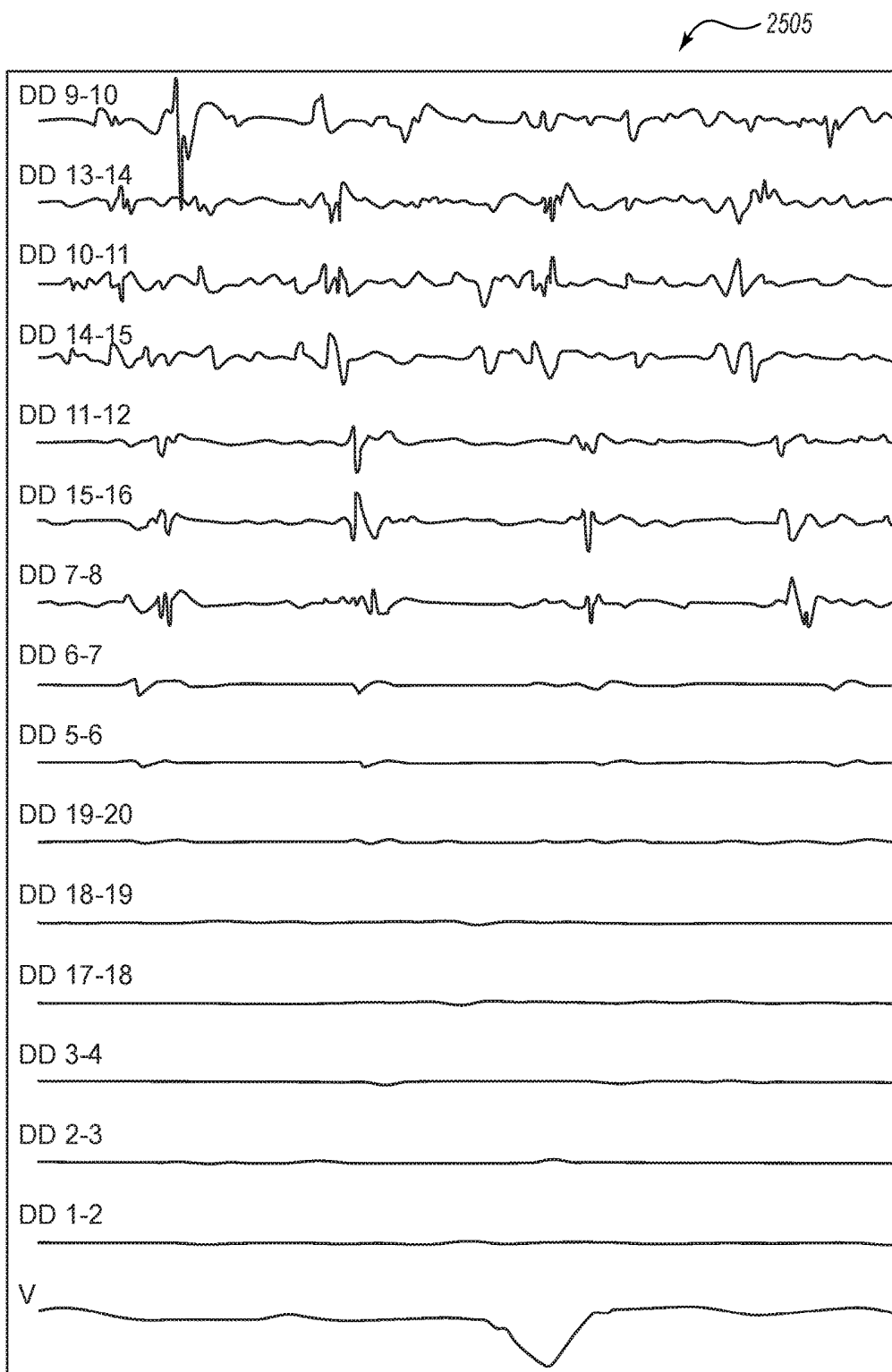


FIG. 48B



FIG. 50A



FIG. 50B

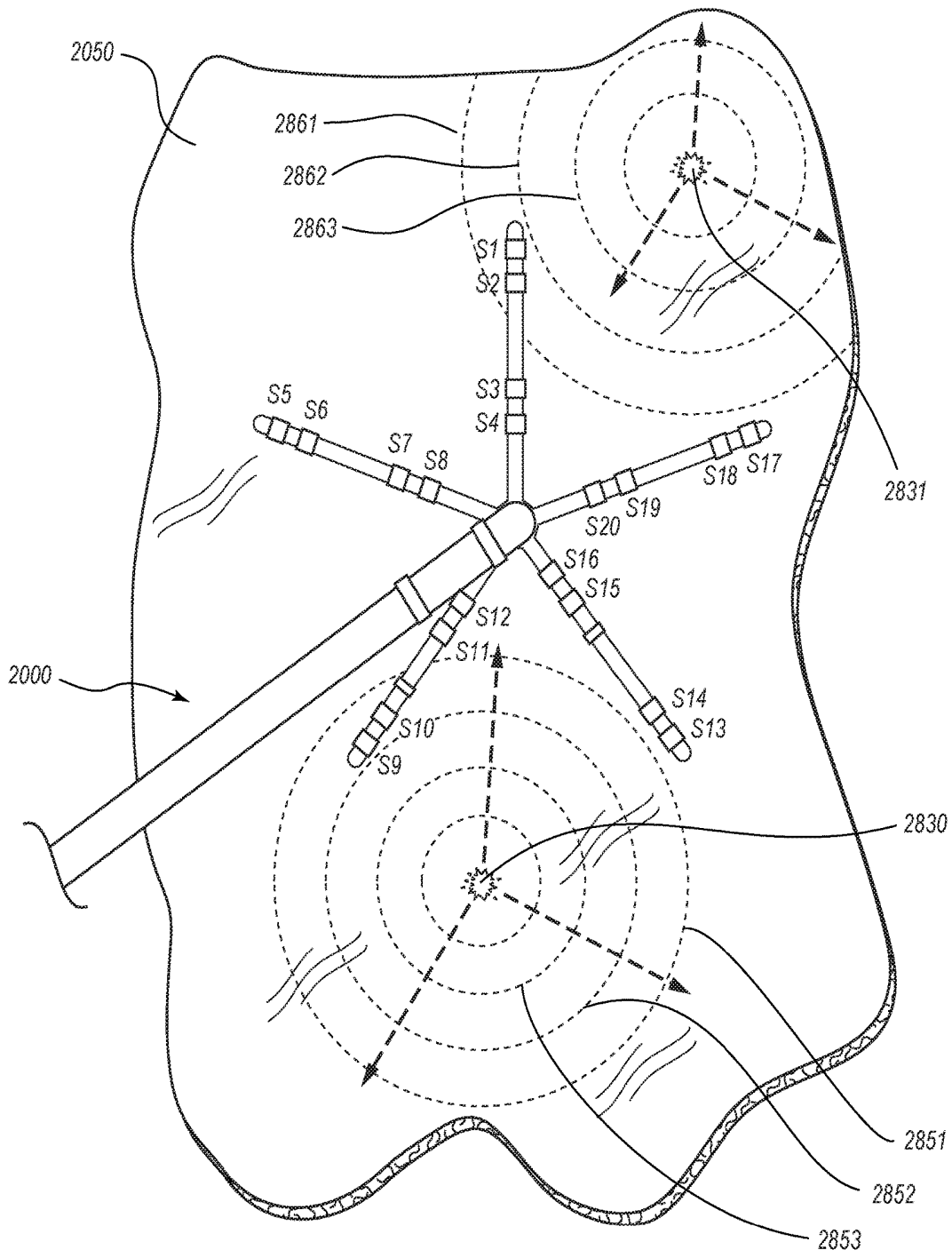


FIG. 51

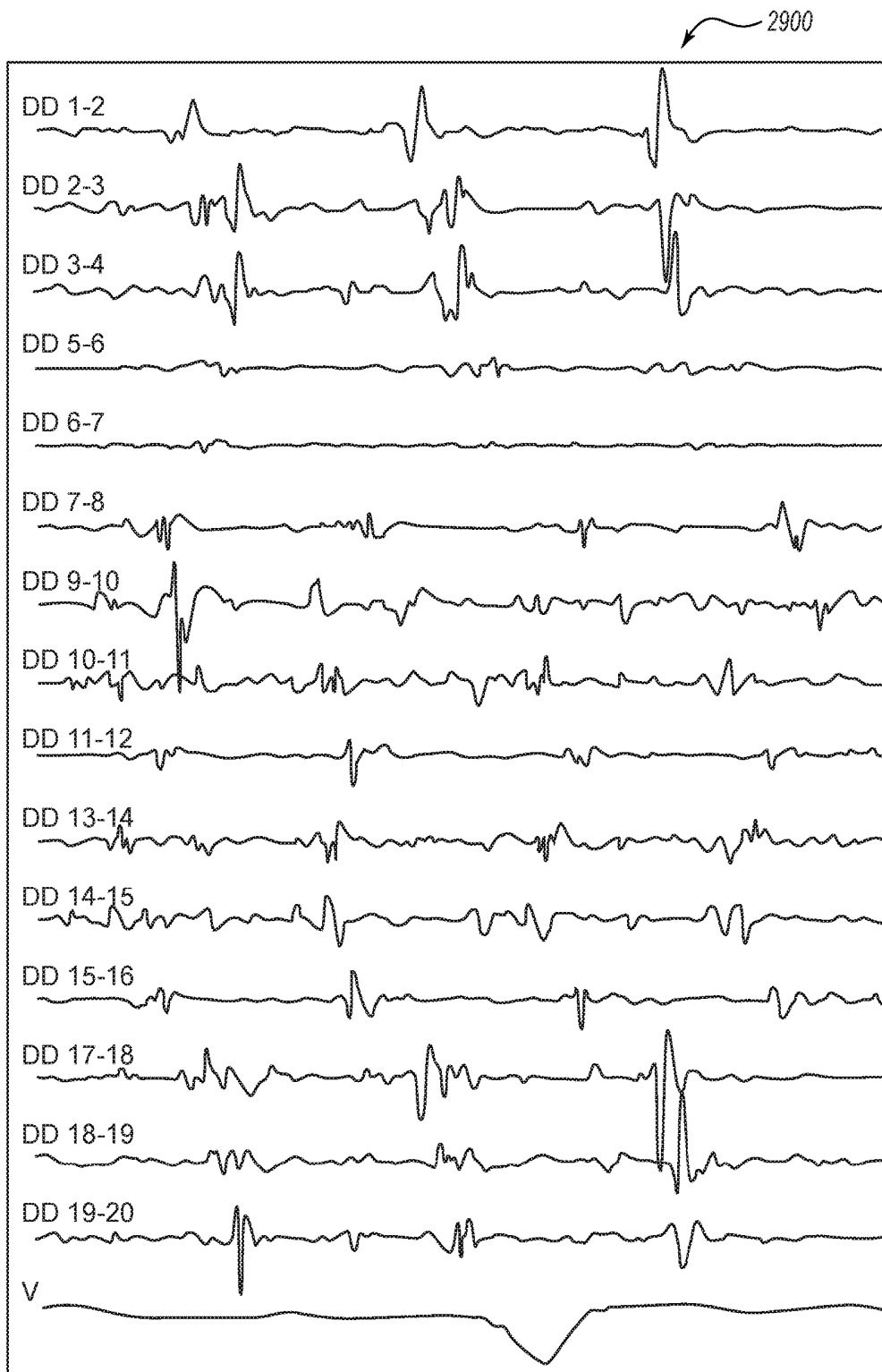


FIG. 52A

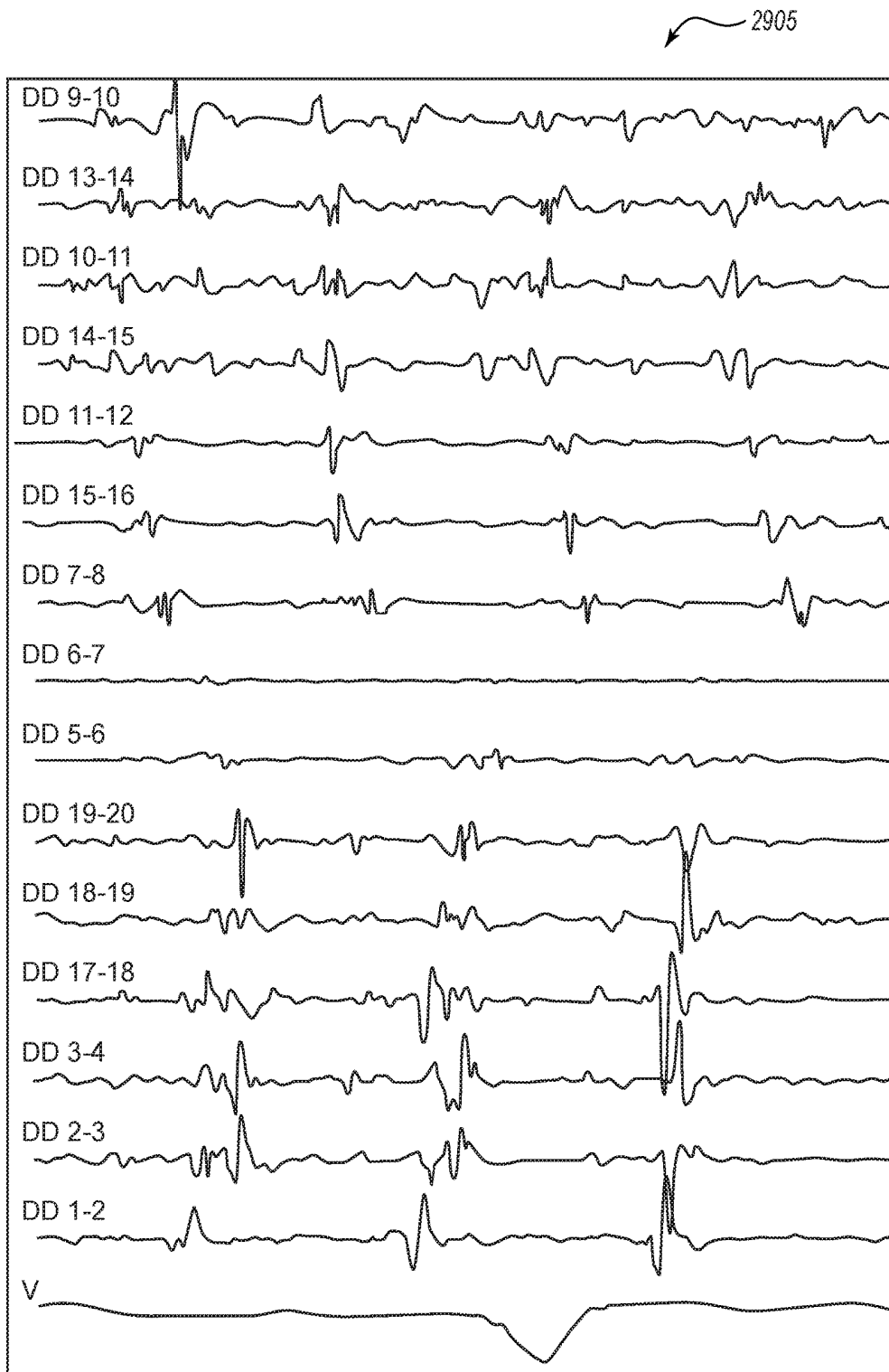


FIG. 52B

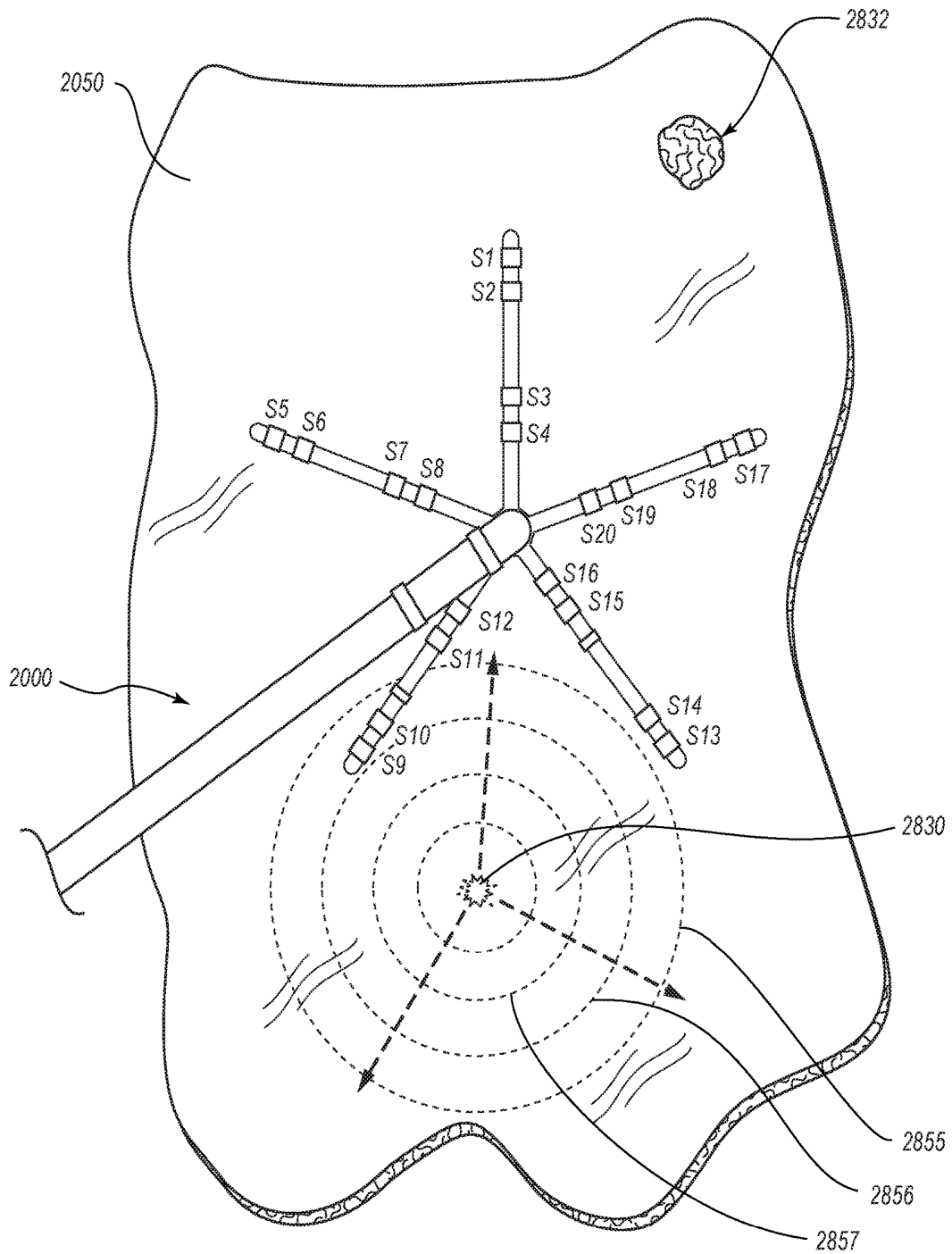


FIG. 53

2910

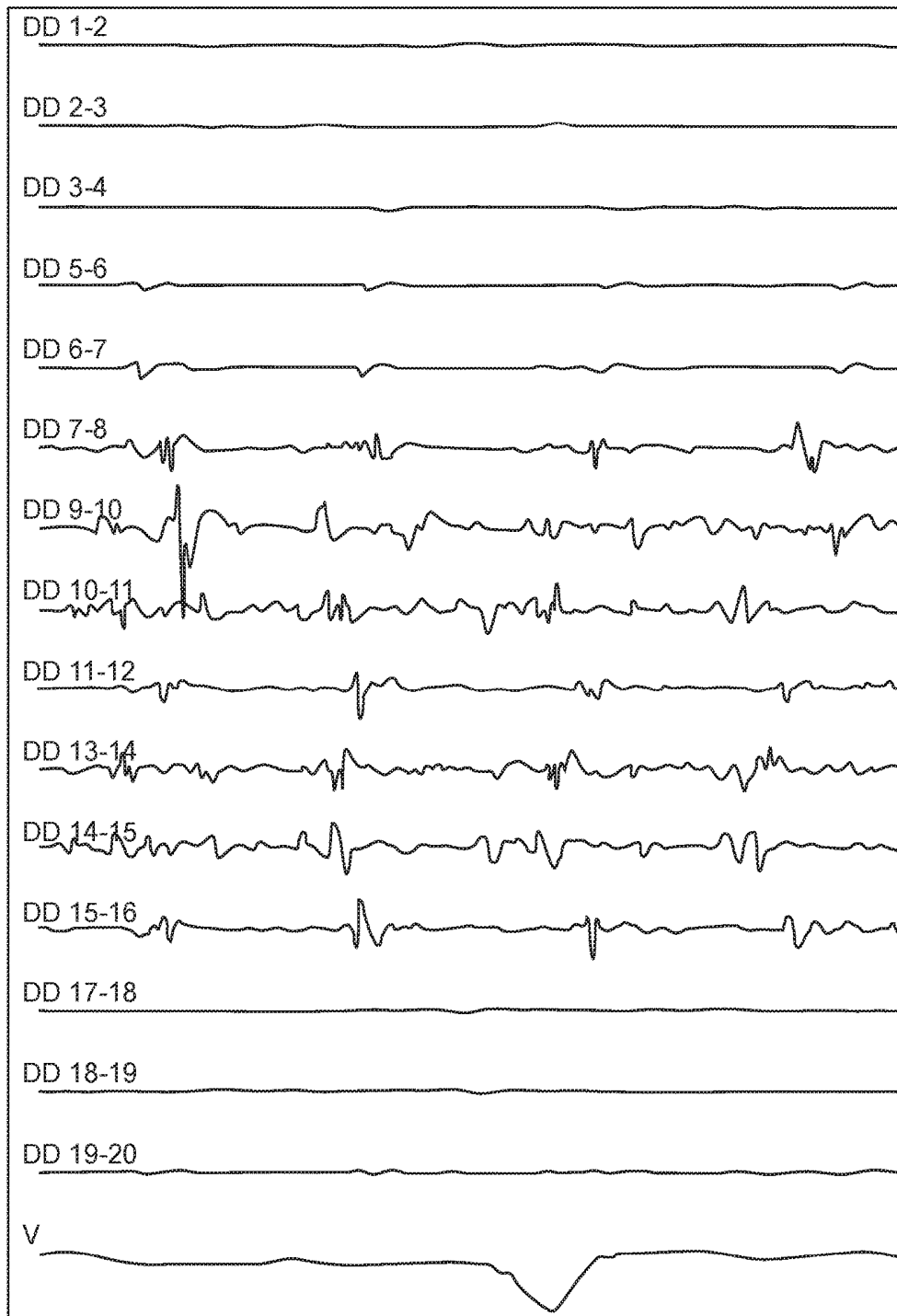


FIG. 54A

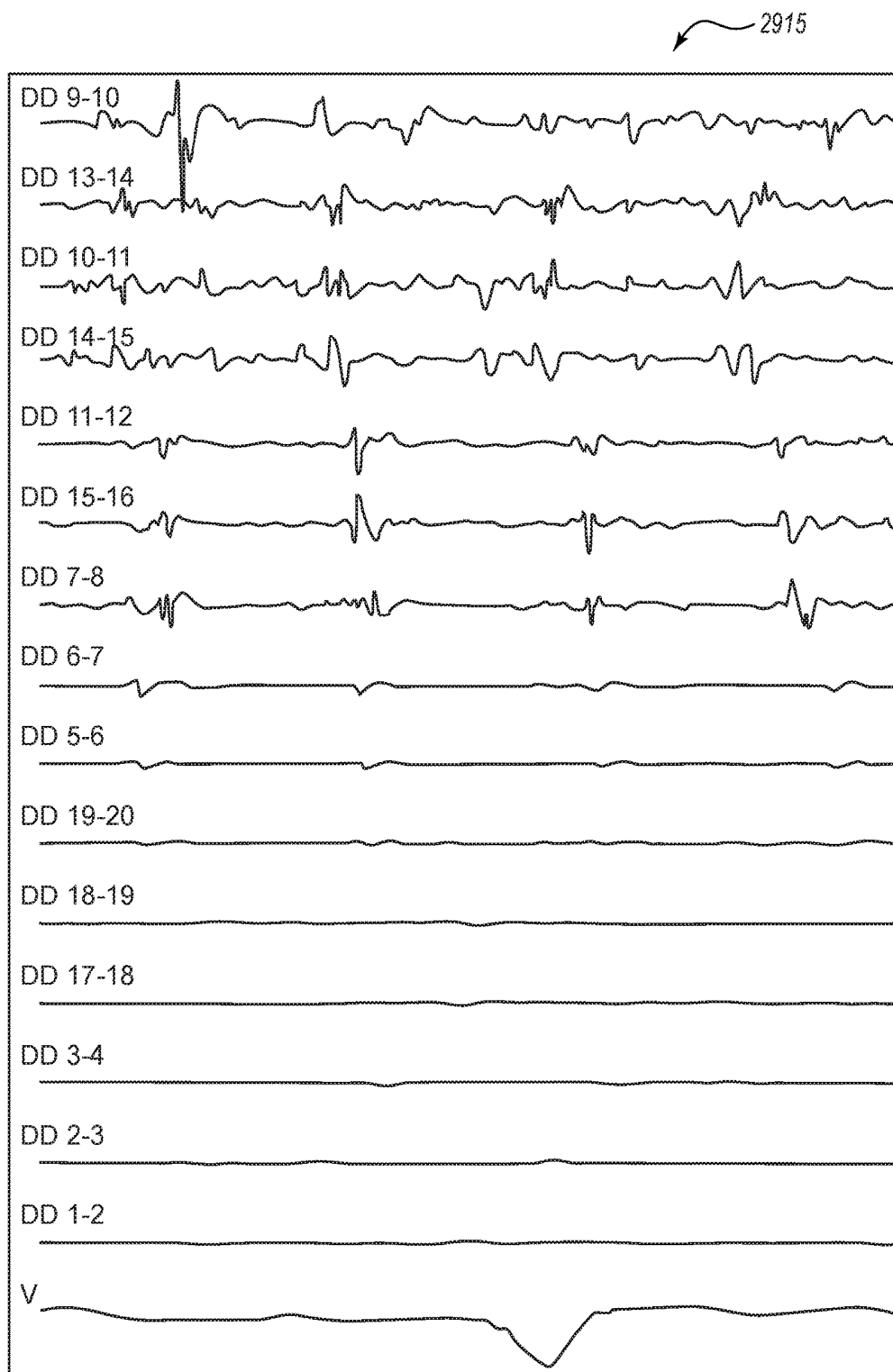


FIG. 54B

ATRIAL FIBRILLATION TREATMENT SYSTEMS AND METHODS

CROSS-REFERENCE TO RELATED APPLICATIONS

This application is a continuation of U.S. patent application Ser. No. 13/923,348, titled ATRIAL FIBRILLATION TREATMENT SYSTEMS AND METHODS, which was filed on Jun. 20, 2013, and which claims the benefit under 35 U.S.C. § 119(e) of U.S. Provisional Patent Application No. 61/662,323, titled ATRIAL FIBRILLATION TREATMENTS, which was filed on Jun. 20, 2012; U.S. Provisional Patent Application No. 61/798,456, titled ATRIAL FIBRILLATION TREATMENTS, which was filed on Mar. 15, 2013; and U.S. Provisional Patent Application No. 61/799,242, titled UPSTREAM APPROACH FOR ABLATION OF ATRIAL FIBRILLATION, which was filed on Mar. 15, 2013, the entire contents of each of which are hereby incorporated by reference herein.

BACKGROUND

Atrial fibrillation (“AF”) is a heart disease that affects a significant portion of the population of the United States (e.g., about 1 to 2 percent in the general population and up to about 10 percent in elderly populations). In a patient with AF, the electrical impulses that are normally generated by the sinoatrial node are overwhelmed by disorganized electrical activity in the atrial tissue, leading to an irregular conduction of impulses to the ventricles that generate the heartbeat. The result is an irregular heartbeat, which may be intermittent or continuous. In human populations, AF-induced irregular heartbeat is a significant source of stroke, heart failure, disability, and death.

There are a number of surgical options available for treating AF. One approach is known as the Cox-Maze III procedure. In this procedure, the left atrial appendage is excised, and a series of incisions and/or cryo- or radiofrequency-lesions are arranged in a maze-like pattern in the atria. The incisions encircle and isolate the pulmonary veins. The resulting scars block the abnormal electrical pathways, improving normal signal transmission and restoring regular heart rhythm. Less invasive techniques are also possible, which may use heating or cooling sources to create impulse-blocking lesions on the heart by ablation rather than incision.

Catheter-based radiofrequency ablation is a particularly common treatment for symptomatic AF, as it is less invasive than surgery. Whether this, or any of the foregoing treatments is used, however, there are certain drawbacks and/or limitations with known techniques. Embodiments discussed below can ameliorate, avoid, or resolve one or more of these drawbacks, as will be apparent from the present disclosure.

BRIEF DESCRIPTION OF THE DRAWINGS

The written disclosure herein describes illustrative embodiments that are non-limiting and non-exhaustive. Reference is made to certain of such illustrative embodiments that are depicted in the figures, in which:

FIG. 1 is a schematic representation of a left and a right atrium with disordered electrical pulses emanating from the pulmonary veins, which may be described as paroxysmal atrial fibrillation.

FIG. 2 is a schematic representation illustrating an ablative treatment for isolating the electrical pulses to resolve the disorder illustrated in FIG. 1.

FIG. 3 is a schematic representation of a left and a right atrium with disordered electrical pulses emanating from the pulmonary veins and also emanating from the atrium wall, or cardiac substrate, which may be described as complex paroxysmal, persistent, or longstanding persistent atrial fibrillation.

FIG. 4 is a schematic representation illustrating an ablative treatment for isolating sources of electrical pulses to resolve the cardiac complex rhythm disorder illustrated in FIG. 3; in some instances, the ablative treatment may be incomplete as drivers of atrial fibrillation may be missed (e.g., not isolated), depending on their location.

FIG. 5 is a schematic representation of a portion of the cardiac substrate, or atrium wall, having multiple atrial drivers that cause atrial fibrillation, particularly more complex types, wherein the atrial drivers generate wavefronts of electrical impulses; the wavefronts are shown in FIG. 5 at a time soon after formation, and the view of FIG. 5 is a schematic enlarged view of a portion of FIG. 3 taken along the view line 5 shown therein.

FIG. 6 is a schematic representation such as that of FIG. 5 illustrating the wavefronts at a later time, wherein wavefronts from various atrial drivers collide with each other, and this collision of wavefronts that were initiated by the drivers can lead to complex and fractionated electrical wavelets.

FIG. 7 is another schematic representation such as that of FIG. 6, but further including anatomical boundaries or scarred regions between the multiple atrial drivers, wherein the wavefronts are shown at a later time than those in FIG. 5, and wherein FIG. 7 illustrates that the atrial drivers generate primary wavefronts that ultimately collide and interact with the anatomic boundaries or scars to generate secondary wavefronts, further impacting the complexity and irregularity of the electrical wavelets.

FIG. 8 is a schematic plot illustrating the electrical signals (point-based assessment of an electrical wave), or waveforms, detected at two different regions of the cardiac substrate shown in FIG. 7 across which the primary and/or secondary wavefronts travel, wherein the upper plot illustrates that the signals generated by collision of wavefronts, collision of wavefronts and scars, and/or collision of wavefronts and anatomic boundaries can be more complex and irregular, and wherein the lower plot illustrates that signals from the initial drivers can be rapid and relatively regular.

FIG. 9 is a schematic illustration of the left atrium, wherein electrical signals are detected at a plurality of regions.

FIG. 10 is a plot illustrating the electrical signal waveforms detected at each of the regions identified in FIG. 9, wherein it can be seen that the different waveforms have different frequencies.

FIG. 11 is a schematic representation illustrating the location mapping of atrial drivers found by ranking electrical signals based on their uniformity and frequency.

FIG. 12 is a schematic representation illustrating an atrial driver isolation procedure to electrically isolate three of the atrial drivers represented in FIG. 11 so as to prevent undesired signals from these drivers from propagating along the atrial wall.

FIG. 13 is a schematic representation illustrating an atrial driver isolation procedure to electrically isolate two of the atrial drivers shown in FIG. 11 in a manner slightly different than that shown in FIG. 12, and further showing a focal ablation procedure to locally isolate a third atrial driver.

FIG. 14A is a flowchart depicting an illustrative method of treating atrial fibrillation.

FIG. 14B is a flowchart depicting another illustrative method of treating atrial fibrillation.

FIG. 14C is a flowchart depicting yet another illustrative method of treating atrial fibrillation.

FIG. 15 is a schematic diagram of an embodiment of a system that can be used to identify one or more atrial drivers.

FIG. 16 is a schematic view of a portion of the system of FIG. 15 that includes a cutaway view of a heart of a patient and a perspective view of an embodiment of a non-contact multi-array sensor positioned in the right ventricle of the heart.

FIG. 17 is a schematic view, similar to FIG. 16, that includes a cross-sectional view of a heart of a patient and a perspective view of a portion of the system of FIG. 15 cross-sectional view of the non-contact multi-array sensor of FIG. 16 deployed in the left atrium of the heart.

FIG. 18 is an enlarged cutaway view of the left atrium of the heart of a patient, similar to FIG. 17, which shows a non-contact multi-array sensor deployed in the left atrium.

FIG. 19 is a diagram of an illustrative output display from the system of FIG. 15.

FIG. 20 is an equivalent circuit of a measurement made by the system of FIG. 15.

FIG. 21 is a diagram of a measurement made by the system of FIG. 15.

FIG. 22 is a display representing the “coherence” measure and the index of hemodynamic performance as determined by the system of FIG. 15.

FIG. 23 is a schematic representation of a non-contact sensor collecting cardiac signals from multiple regions or volumes and interpolating the signals to locations on the cardiac substrate or atrial wall.

FIG. 24 is a display representing the cardiac signals, specifically electrograms, obtained via an arrangement such as shown in FIG. 23 and their identified associated regions on the cardiac substrate or atrial wall.

FIG. 25A is a schematic cross-sectional view of a portion of another embodiment of a system for identifying one or more atrial drivers, wherein the system includes a multi-sensor array that is shown in a constricted or non-deployed state.

FIG. 25B is another schematic cross-sectional view of the portion of the system shown in FIG. 25A, wherein the multi-sensor array is in an expanded or deployed state such that sensors thereof are in contact with the atrial wall.

FIG. 26 is a schematic cross-sectional view of a portion of another embodiment of a system for identifying one or more atrial drivers, wherein the system includes a multi-sensor array that is positioned at an exterior of the patient.

FIGS. 27A-27D depict illustrative instrumentation and methods for obtaining trace electrograms associated with the heart.

FIG. 28 is a schematic representation of an illustrative method by which a non-contact sensor collects cardiac signals from multiple regions of the cardiac substrate or atrial wall.

FIG. 29 is a flowchart depicting an illustrative method of treating atrial fibrillation.

FIG. 30 is a plot depicting an electrocardiogram of a patient who has a sinus rhythm with intermittent suppression by a repetitive slow atrial driver, along with a simplified electrocardiogram in which only the major voltage peaks are represented.

FIG. 31 is a plot depicting an example of a sinus rhythm electrocardiogram, along with a simplified electrocardiogram in which only the major voltage peaks are represented.

FIG. 32A is a schematic representation of a portion of a cardiac substrate, or atrium wall, having a primary atrial driver that generates a regular series of wavefronts of electrical impulses that propagate toward a secondary atrial driver, which may also be referred to as a bystander driver, that is suppressed.

FIG. 32B is a schematic plot illustrating the electrical signals (point-based assessment of an electrical wave), or wavefronts or waveforms, detected at a region of the cardiac substrate designated by a hexagon in FIG. 32A illustrating that the signals generated by the driver are regular and have a predictable, repeated period.

FIG. 33A is a schematic representation of another portion of a cardiac substrate having a primary atrial driver that generates a regular series of wavefronts of electrical impulses that propagate toward a secondary atrial driver, wherein the secondary atrial driver is stable and not suppressed by the primary driver, and likewise generates a regular series of wavefronts of electrical impulses that propagate toward the primary atrial driver, wherein a frequency of the wavefronts produced by the secondary atrial driver is lower than a frequency of the wavefronts produced by the primary atrial driver.

FIG. 33B is a schematic plot illustrating the electrical signals (e.g., waveforms) detected at a region of the cardiac substrate designated by a hexagon in FIG. 33A illustrating that the signals generated by the drivers are regular and have a predictable, repeated period and neither set of waveforms produced by either driver suppresses operation of the other driver.

FIG. 34A is a schematic representation of another portion of a cardiac substrate having a primary atrial driver that generates a regular series of wavefronts of electrical impulses that propagate toward a secondary atrial driver, wherein the secondary atrial driver is stable and likewise generates a regular series of wavefronts of electrical impulses that propagate toward the primary atrial driver, wherein a frequency of the wavefronts produced by the secondary atrial driver is lower than a frequency of the wavefronts produced by the primary atrial driver, and wherein every third wavefront produced by the secondary atrial driver suppresses what would be every fourth wavefront of the primary driver.

FIG. 34B is a schematic plot illustrating the electrical signals (e.g., waveforms) detected at a region of the cardiac substrate designated by a hexagon in FIG. 34A demonstrating the periodic suppression of primary wavefronts due to activity of the stable secondary driver.

FIG. 35A is a schematic representation of another portion of a cardiac substrate having a primary atrial driver that generates a regular series of wavefronts of electrical impulses that propagate toward a secondary atrial driver, wherein the secondary atrial driver functions intermittently, and thus the two operational modes of the secondary driver are designated by alternative scenarios (as indicated by the recitation “OR”); wherein in the upper alternative, the secondary atrial driver is dormant, and thus the primary atrial driver is permitted to generate its electrical wavefronts, and in the lower alternative, the secondary atrial driver is temporarily active and generates a standalone or irregular wavefront that temporarily suppresses generation of a wavefront by the primary driver (which is indicated in the upper alternative by intermittent broken lines where wavefronts would be expected).

FIG. 35B is a schematic plot illustrating the electrical signals (e.g., waveforms) detected at a region of the cardiac substrate designated by a hexagon in FIG. 35A illustrating

the periodic suppression of primary wavefronts due to activity of the intermittent secondary driver.

FIG. 36 is a schematic depiction of a portion of an illustrative method for identifying drivers from a trace electrocardiogram, wherein unique frequencies are isolated to identify dominant drivers.

FIG. 37 is a schematic representation of another portion of a cardiac substrate having an atrial driver that is spaced from a series of five different sensors by varying amounts, wherein each sensor is represented by a numbered hexagon.

FIG. 38A is a schematic plot illustrating the electrical signals (e.g., waveforms) that may be detected by each of the sensors shown in FIG. 37 when the atrial driver is a primary driver from which wavefronts regularly propagate outwardly.

FIG. 38B is a schematic plot illustrating the electrical signals (e.g., waveforms) that may be detected by each of the sensors shown in FIG. 37 when the atrial driver is a secondary driver that has a lower frequency than a neighboring driver (e.g., a neighboring primary driver) and/or that generates wavefronts intermittently, such that wavefronts are shown initially propagating outwardly relative to the innermost sensor, but thereafter wavefronts are shown propagating inwardly toward the innermost sensor.

FIG. 39 is a plan view of an embodiment of a sensor assembly that includes multiple contact sensors that can extend along a cardiac substrate in at least two orthogonal directions, or stated otherwise, in at least two dimensions, to define at least a two-dimensional sensing area, wherein the sensor assembly is depicted in operation adjacent to a cardiac wall.

FIG. 40 is a plan view of another embodiment of a sensor assembly that includes multiple contact sensors that can extend along a cardiac substrate in at least two orthogonal directions, or stated otherwise, in at least two dimensions, to define at least a two-dimensional sensing area, wherein the sensor assembly is depicted in operation adjacent to a cardiac wall.

FIG. 41 is a flowchart depicting an illustrative method of treating atrial fibrillation.

FIG. 42 is a flowchart depicting another illustrative method of treating atrial fibrillation.

FIG. 43 is a plan view of an embodiment of a sensor assembly in the process of gathering electrograms from a portion of an atrial wall, wherein a driver is within a sensing region of the sensor assembly.

FIG. 44A is a plot that includes electrograms gathered via the sensor assembly and that also shows a base signal of the heart.

FIG. 44B is a plot that includes the electrograms from FIG. 44A in a rearranged format to demonstrate propagation of wavefronts from the driver.

FIG. 45 is a plan view of an embodiment of a sensor assembly in the process of gathering electrograms from a portion of an atrial wall, wherein two separate drivers are within a sensing region of the sensor assembly.

FIG. 46A is a plot that includes electrograms gathered via the sensor assembly and that also shows a base signal of the heart.

FIG. 46B is a plot that includes the electrograms from FIG. 46A in a rearranged format to demonstrate propagation of wavefronts from the drivers.

FIG. 47 is a plan view of an embodiment of a sensor assembly in the process of gathering electrograms from a portion of an atrial wall, wherein a driver is external to a sensing region of the sensor assembly.

FIG. 48A is a plot that includes electrograms gathered via the sensor assembly and that also shows a base signal of the heart.

FIG. 48B is a plot that includes the electrograms from FIG. 48A in a rearranged format to demonstrate propagation of wavefronts from the driver.

FIG. 49 is a plan view of an embodiment of a sensor assembly in the process of gathering electrograms from a portion of an atrial wall, wherein a first driver is at an exterior of the sensing region of the sensor assembly and a second driver is within the sensing region of the sensor assembly.

FIG. 50A is a plot that includes electrograms gathered via the sensor assembly and that also shows a base signal of the heart.

FIG. 50B is a plot that includes the electrograms from FIG. 50A in a rearranged format to demonstrate propagation of wavefronts from the drivers.

FIG. 51 is a plan view of an embodiment of a sensor assembly in the process of gathering electrograms from a portion of an atrial wall, wherein two drivers are near a sensing region of the sensor assembly but neither driver is within the sensing region.

FIG. 52A is a plot that includes electrograms gathered via the sensor assembly and that also shows a base signal of the heart.

FIG. 52B is a plot that includes the electrograms from FIG. 52A in a rearranged format to demonstrate propagation of wavefronts from the driver.

FIG. 53 is a plan view of an embodiment of a sensor assembly in the process of gathering electrograms from a portion of an atrial wall, wherein one driver is near a sensing region of the sensor assembly and another portion of the atrial wall that previously acted as a driver has been ablated and no longer emits wavefronts.

FIG. 54A is a plot that includes electrograms gathered via the sensor assembly and that also shows a base signal of the heart.

FIG. 54B is a plot that includes the electrograms from FIG. 44A in a rearranged format to demonstrate propagation of wavefronts from the driver.

DETAILED DESCRIPTION

As noted above, many procedures for treating AF involve creating a pattern of lesions around the pulmonary veins so as to electrically isolate the pulmonary veins. Further lesion patterns may also be used to block other errant, irregular, problematic, or otherwise undesired electrical signals. The procedures are often quite lengthy and may be protracted or otherwise complicated when it is difficult to determine a location on the heart from which the problematic electrical signals emanate.

Catheter-based radiofrequency ablation is an example of an established treatment for symptomatic AF, and can involve the creation of lesions as just described. Success rates can vary depending on the AF subtype. For example, for paroxysmal AF, a success rate of 70%-85% may be common, as the disease predominantly involves pulmonary or great vein triggers. Stated otherwise, the high success rate may be achievable because the pulmonary or great vein triggers may be readily isolated by creating blocking lesions around the pulmonary veins. In contrast, persistent AF and longstanding persistent AF may have a lower success rate (e.g., 4%-60%), as the disease may involve not only primarily venous triggers, but also scars and/or multiple drivers within the left and right atria. As used herein, the term

“driver” refers to any location, area, or region on or in the heart that is a source of AF signals. A driver can comprise, for example, a focal trigger, a substrate trigger, or a ganglion plexus; or stated otherwise, a driver can comprise a malfunctioning autonomic cell bundle. Drivers may also be referred to as focal drivers.

Disclosed herein are methods, systems, and devices for identifying, locating, and/or treating such drivers (e.g., malfunctioning autonomic cell bundles) to treat AF. In some embodiments, an electrophysiology apparatus is used to measure electrical activity occurring in a heart of a patient and/or to visualize the electrical activity and/or information related to the electrical activity. Other or further embodiments include a methodology for mapping the heart so as to identify a driver. Still further embodiments include a methodology for sorting or ranking electrograms to determine a position of a driver. Some embodiments include treating a patient via ablation at or near an identified driver. Various embodiments increase the effectiveness of AF treatment and/or reduce overtreatment of patients (e.g., by avoiding the creation of lengthy and/or complicated scars).

FIG. 1 is a schematic representation of a left atrium 102 and a right atrium 104 with disordered electrical pulses emanating from drivers 105, 106, 107, 108 (which are schematically represented by starbursts) in the pulmonary veins 115, 116, 117, 118, respectively. FIG. 1 may be described as illustrating paroxysmal atrial fibrillation.

FIG. 2 is a schematic representation illustrating an ablative treatment for isolating the electrical pulses to resolve the disorder illustrated in FIG. 1. In particular, a first ablation path 120 surrounds and isolates the drivers 105, 106 and the pulmonary veins 115, 116, and a second ablation path 122 surrounds and isolates the drivers 107, 108 and the pulmonary veins 117, 118.

FIG. 3 is a schematic representation of another example of a left atrium 102 and a right atrium 104 with disordered electrical pulses emanating from the pulmonary veins 115, 116, 117, 118 and also emanating from the atrium wall 124, or cardiac substrate. In particular, the disordered electrical pulses can emanate from multiple drivers 131, 132, 133, 134, 135, 136, 137, 138, as well as the drivers 105, 106, 107, 108. FIG. 3 may be described as illustrating persistent or longstanding persistent atrial fibrillation.

FIG. 4 is a schematic representation illustrating an ablative treatment for isolating sources of electrical pulses to resolve the cardiac complex rhythm disorder illustrated in FIG. 3. Ablation paths 120, 122 can be formed to isolate the pulmonary veins 115, 116 and 117, 118, respectively, along with their associated drivers 105, 106, 107, 108. One or more additional ablation paths 140, 142, 144 can also be formed. These ablation paths 140, 142, 144 can be used to block problematic electrical pulses emanating from the drivers 131, 132, 133, 134, 135, 136, 137, and 138.

FIGS. 1-4 illustrate principles that are generally known. For example, the ablation paths 120, 122, 140, 142, 144 can be formed in any suitable manner. Standard ablation treatments may be used, such as limited pulmonary vein isolation (PVI), wide-area or antral pulmonary vein isolation (APVI), and/or complex fractionated atrial electrogram (CFAE) ablation. FIGS. 5-13, however, illustrate new and/or further approaches for treating cardiac complex rhythm disorders. FIGS. 5-10 illustrate concepts for locating problematic drivers on or within the heart, which can be treated in manners such as illustrated in FIGS. 12 and 13. While the concepts discussed with respect to FIGS. 5-10 can aid in explaining how or why certain methods and systems described herein may be effective, it is to be understood that these concepts

are non-limiting. Stated otherwise, the present disclosure—including the disclosure of methods and systems for the treatment of AF—is not bound or limited by theories or explanations relative thereto that are set forth herein.

FIG. 5 is a schematic representation of a portion of the cardiac substrate 150, or atrium wall, having multiple atrial drivers 133, 134, 135, 136 that each generates multiple wavefronts of electrical impulses. Wavefronts 153, 154, 155, 156 are depicted as circles of a larger diameter, and additional wavefronts generated thereafter, which are depicted as circles at the interior of the wavefronts 153, 154, 155, 156. The drivers 133, 134, 135, 136 can cause atrial fibrillation, and the atrial wall can transmit the errant, erroneous, or irregular signal in the same manner that they conduct regular or desirable signals. The wavefronts detected via the electrograms can be used to identify the positions at which the undesired signals originate. In FIG. 5, the wavefronts 153, 154, 155, 156 are shown at a time soon after formation. The drivers 133, 134, 135, 136 can each be repetitive, each continually initiating stable wavefronts. Stated otherwise, the drivers 133, 134, 135, 136 may be stable so as to regularly generate electrical waveforms that propagate outwardly and that have stable or substantially constant periodicities.

FIG. 6 is a schematic representation of a portion of the cardiac substrate 150, such as that of FIG. 5, illustrating the wavefronts 153, 154, 155, 156 at a later time. The wavefronts 153, 154, 155, 156 from corresponding atrial drivers 133, 134, 135, 136 collide with each other. As a result, portions of the cardiac substrate 150 positioned between the drivers 133, 134, 135, 136 encounter complex electrical signals. The signals may be noisy, and may be sporadic or irregular, as wavefronts from the multiple atrial drivers 133, 134, 135, 136 may arrive with irregular and/or offset timing.

FIG. 7 illustrates a different cardiac substrate 150' that includes anatomical boundaries and/or damaged tissue 161, 162, 163 (e.g., scarred regions, such as from prior ablative procedures and/or degenerative heart ailment), which may more generally be referred to as boundary structures, between the multiple atrial drivers 133, 134, 135, 136. The primary wavefronts 153, 154, 155, 156 generated by the drivers 133, 134, 135, 136 can ultimately collide and interact with the boundary structures 161, 162, 163 to yield secondary wavefronts. For example, secondary wavefronts 166, 167 may result from interaction of a primary wavefront, which is generated by the driver 133, with the boundary structure 161. As a result, portions of the cardiac substrate 150' positioned between the drivers 133, 134, 135, 136 encounter complex electrical signals. The signals may be noisy, and may be sporadic or irregular, as wavefronts from the multiple atrial drivers 133, 134, 135, 136, as well as from the boundary structures 161, 162, 163 may arrive with irregular and/or offset timing.

Three regions or positions 170, 171, 175 in the cardiac substrate 150' are shown in FIG. 7. The positions are schematically represented by hexagons, although the regions may not necessarily be hexagonal in shape. The electrical signals encountered at the positions 170, 171 are illustrated in FIG. 8.

In particular, FIG. 8 is a schematic plot 172 illustrating the voltage *V* of the electrical signals, or waveforms, as a function of time, as detected at the positions 170, 171 of the cardiac substrate 150'. Although the waveforms are depicted with discrete pulses (e.g., showing a point-based assessment of an electrical wave), in other instances, the waveforms appear more wavelike (e.g., such as shown in FIG. 24). As can be appreciated from the plot that corresponds to the

position **170**, complex fractionated electrograms can be associated with regions of marked electrical variability. Stated otherwise, marked activation shifts can represent collisions of waveforms at a position that is remote from one or more drivers. Accordingly, more complex and/or irregular waveforms can be associated with regions that are remote from one or more drivers. As can be appreciated from the plot that corresponds to the position **171**, waveforms that are stable (e.g., relatively regular) and that are rapid (e.g., have a high frequency) can be associated with regions that are at or near a driver.

FIG. **9** is a schematic illustration of the left atrium **102**, wherein electrical signals are detected at a plurality of positions **180, 181, 182, 183, 184, 185**. Any suitable system and/or device may be used to detect the signals at the plurality of positions. More or fewer positions may be detected than the six shown and/or the detections may be simultaneous. In other or further instances, detection of electrical signals at each of the positions may be carried out individually or in groups, such as by passing a sensor over one or more of the positions at a time.

Illustrative examples of sensing systems and devices that are suitable for detecting the electrical signals the correspond with the positions **180, 181, 182, 183, 184, 185** are discussed further below. For example, in some embodiments, a sensor, which may also be referred to as a sensor system or a or a sensor array, can be positioned within the left atrium **102**. An illustrative example of such a sensor array is shown in FIGS. **16-18**. The sensor array may be spaced from the inner atrial wall and may be capable of substantially simultaneously mapping electrical properties (e.g., electrogram waveforms) at numerous regions of the left atrium **102**. The sensor array may similarly be positioned with the right atrium **104** to detect electrical signals corresponding to positions along the inner atrial wall of the right atrium **104**. In some instances, the same sensor array is used in either atrium **102, 104**, whereas in other embodiments, multiple sensor arrays may be used. The one or more sensor arrays may collect data from both atria **102, 104** simultaneously, or they may collect the data serially.

In other or further embodiments, a sensor system, such as one or more of the sensor arrays depicted in FIGS. **25A** and **25B**, may be positioned at the interior of the left atrium **102** and/or the right atrium **104**, and the sensor system may include multiple sensors that are placed in contact with the inner atrial walls. The sensors may be configured to detect electrical signals conducted along the wall of the cardiac substrate over time (e.g., electrogram waveforms) at the portions of the atrial wall with which they are in contact.

In still other or further embodiments, electrical signals corresponding with a various portions of the cardiac substrate, such as the plurality of positions **180, 181, 182, 183, 184, 185** of FIG. **9**, may be obtained via a sensor system having one or more sensors positioned at an exterior surface of the heart and/or protruding into a wall of the heart. For example, in some embodiments, one or more sensors may be positioned within the body of the patient and/or external to chambers of the heart.

In other or further embodiments, electrical signals corresponding with a various portions of the cardiac substrate, such as the plurality of positions **180, 181, 182, 183, 184, 185** of FIG. **9**, may be obtained via a sensor system positioned at an exterior of the patient, such as at the skin surface of the patient. One illustrative example of such a sensor system is depicted in FIG. **26**. The sensor system may

include skin electrodes or any other suitable sensor device or devices, and data collection via the sensors can include body surface mapping.

In still further instances, more localized sensing may be achieved via sensors such as those depicted in FIGS. **39, 40, and 43**. For example, in various instances, a sensor may be positioned at the end of a catheter (e.g., a steering catheter), which may be positioned within an atrium adjacent to the cardiac wall. In some instances, the sensor may be held in place for a time sufficient to observe and/or obtain a suitable reading of the electrical activity of the portion of the heart against which the sensor is pressed (e.g., a fraction of a second, several seconds, a minute or less), and the sensor may then be swept or otherwise relocated to other portions of the heart.

As can be appreciated from the foregoing, any suitable sensor system, which may include one or more sensing devices, can be used to obtain electrical signals that are associated with various positions on the heart, such as the positions **180, 181, 182, 183, 184, 185** on the left atrium **102**, as shown in FIG. **9**. The electrical signals may correspond with or otherwise be representative of electrical signals conducted along the wall of the cardiac substrate over time (e.g., electrogram waveforms). However, in some embodiments, the electrical signals may include data from which electrogram waveforms can be determined. Stated otherwise, the electrical signals may include electrogram waveform information, and the electrogram waveforms may be determined from this information. In various embodiments, suitable sensor systems for obtaining electrogram waveform information include one or more of a sensor array balloon, a basket mapping catheter and/or any other type of mapping catheter, and an expandable mesh catheter (each of which may be positioned within the heart of the patient) and skin electrodes (which may be positioned at an exterior of the patient).

FIG. **10** is a plot **188** illustrating the electrical signal waveforms detected at each of the regions **180, 181, 182, 183, 184, 185** identified in FIG. **9**. The different waveforms can have different frequencies. In the illustrated embodiment, all of the waveforms are generally stable, with regular periodicities. It can be visually ascertained that the waveform associated with the position **180** has the highest frequency (shortest period), and thus, of all of the regions **180, 181, 182, 183, 184, 185**, the region **180** may be the closest to, or most likely to correspond with, a driver.

As previously noted, all of the waveforms in FIG. **10** are generally stable or periodic. In other instances, one or more of the waveforms may be complex and/or irregular. In some methods for determining a location of a driver, the complex and/or irregular waveforms can be eliminated or discounted as potential driver positions.

Any suitable method for analyzing and/or ranking waveforms may be used to identify one or more driver positions. For example, in some embodiments, waveforms can be ranked, as to their likelihood of corresponding to a driver position, based on their complexity (or lack thereof) and/or their frequency. Some methods rank the waveforms based on both a complexity score and/or frequency. In some embodiments, complexity may be determined via Fourier analysis (e.g., Fast Fourier Transform (FFT) analysis). A complexity score may be assigned based on the number of and/or some other property related to the constituent waves of the complex waveform. In some embodiments, high complexity and low frequency yield low rankings, whereas low complexity and high frequency yield high rankings. Rankings may be achieved via a weighting algorithm. For example, high

frequencies and/or low complexities may be weighted higher than low frequencies and/or high complexities.

In other or further embodiments, one or more other factors may be incorporated into the ranking of potential driver sites. For example, in some instances, it may be assumed that multiple driver sites are present if there are multiple positions that yield high rankings, and if these positions are spaced from each other. This assumption may be even stronger if there are lower-ranked positions that are physically situated between the highly ranked positions. For example, the lower-ranked positions may have more complex waveforms than those associated with the highly ranked positions. By way of illustration, with reference again to FIG. 7, the positions 171 and 175 may be more likely to be at or near drivers (i.e., the drivers 135, 134, respectively), since these positions 171, 175 yield regular waveforms with relatively high frequencies. In some ranking or sorting algorithms, the likelihood that one or more of the positions 171, 175 may be at or near drivers may be augmented by the fact that the position 170 is situated between them and yields a complex waveform (as depicted in FIG. 8). Accordingly, in some embodiments, a ranking algorithm may assign additional weight to potential driver positions if lower-ranked areas are physically situated between the driver positions. In other or further embodiments, waveform amplitude may be used as a parameter in the ranking criteria. However, in some instances and/or for some sensing systems, amplitude may be a less useful ranking criteria as amplitude can be affected by poor electrical contact with the heart tissue. In various embodiments, one or more, two or more, or three or more of waveform unity, frequency, amplitude, and position (e.g., the position on the heart with which the waveform is associated) may be used as parameters in the ranking criteria. As discussed further below, other waveform criteria may also be used to rank signals as to their proximity to a driver and/or to determine whether signals are likely to have originated from the same or different drivers. For example, in some embodiments, a shape of the waveform, such as whether a slope thereof is initially positive or negative, the sharpness and/or number of peaks or valleys, etc., can be used to distinguish signals that originate from different drivers.

Any suitable algorithms may be used to rank the waveforms and their associated positions for likelihood of association with a driver. In some embodiments, the algorithms may be implemented by a practitioner, such as by visually observing or reviewing electrograms. The electrograms, for example, may be provided side-by-side on a display, and the practitioner might observe one or more properties of the waveforms to determine that a position on the heart associated with one or more of the waveforms is in proximity to a driver. In other or further embodiments, the algorithms may be implemented by a computer and/or dedicated hardware. In general, at least some portions of the subject matter disclosed herein may be described herein in terms of various functional components and processing steps. A skilled artisan will appreciate that such components and steps may be implemented as any number of hardware or software components or combination thereof configured to perform the specified functions. For example, an exemplary embodiment may employ various graphical user interfaces, software components, and database functionality.

For the sake of brevity, conventional techniques for computing, data entry, data storage, networking, and/or the like may not be described in detail herein. Furthermore, the connecting lines shown in various figures contained herein (e.g., FIG. 15) are intended to represent exemplary func-

tional relationships and/or communicative, logical, and/or physical couplings between various elements. A skilled artisan will appreciate, however, that many alternative or additional functional relationships or physical connections may be present in a practical implementation of a system or method for treating AF.

Additionally, principles of the present disclosure may be reflected in a computer program product on a computer-readable storage medium having computer-readable program code means embodied in the storage medium. Any suitable tangible, nontransitory computer-readable storage medium may be utilized, including magnetic storage devices (hard disks, floppy disks, and the like), optical storage devices (CD-ROMs, DVDs, Blu-Ray discs, and the like), flash memory, and/or the like. These computer program instructions may be loaded onto a general purpose computer, special purpose computer, or other programmable data processing apparatus to produce a machine, such that the instructions that execute on the computer or other programmable data processing apparatus create means for implementing the functions specified. These computer program instructions may also be stored in a computer-readable memory that can direct a computer or other programmable data processing apparatus to function in a particular manner, such that the instructions stored in the computer-readable memory produce an article of manufacture including implementing means which implement the function specified. The computer program instructions may also be loaded onto a computer or other programmable data processing apparatus to cause a series of operational steps to be performed on the computer or other programmable apparatus to produce a computer-implemented process, such that the instructions which execute on the computer or other programmable apparatus provide steps for implementing the functions specified.

FIG. 11 is a schematic representation illustrating the location mapping of atrial drivers found by ranking electrical signals based on their uniformity and frequency. In some embodiments, FIG. 11 may correspond with a display 190 on which a representative image 191 of the heart is displayed to a practitioner. The representative image 191 may simulate a 3-dimensional model of the heart, or a portion thereof. For example, 3-dimensional mapping may be performed. In some embodiments, the potential driver positions 192p, 193p, 194p, 195p may be shown on the display 190. In some embodiments, the rank or weight of each driver position 192p, 193p, 194p, 195p may also be shown, such as by color, grayscale, or any other suitable visual indicator. In some embodiments, the representative image 191 may be multicolored, with the color scale corresponding to driver ranking or likelihood of driver position. For example, the image 191 may comprise an isochronal map of at least a portion of the heart. As colored, the representative image 191 may provide a 4-dimensional map of the heart, with the three physical dimensions being overlaid with one or more colors representative of the fourth dimension (such as driver ranking, likelihood of driver position, signal frequency, etc.). In some embodiments, the coloring may be determined by one or more of waveform stability and frequency for a given position on the heart. Accordingly, a practitioner may be able to readily identify the positions that are likely associated with drivers, such as by looking for one or more "hot spots" on the image 191 and/or one or more positions that are flagged as being potential driver positions. In further embodiments, the waveforms generated at multiple positions may also be shown on the display 190 (e.g., in a manner similar to that illustrated in FIG. 24). In some

embodiments, a practitioner may edit the image **191**, such as by adding a desired color, symbol, and/or other indicator at one or more positions on the image **191** to indicate any desired property, such as likelihood of being (or being near) a driver. In other or further embodiments, a computer program or other machine-implemented algorithm may automatically assign one or more colors, symbols, and/or other indicators to the image **191**.

In some embodiments, atrial electrograms (such as shown in FIGS. **10** and **24**) can be collected in real time and an isochronal mapping of the heart based on the electrograms (such as shown in FIG. **11**) can be provided. For example, the image **191** may be provided on a screen that is observable to a practitioner. As further discussed below, in some embodiments, the mapping is achieved via non-contact sensors within the heart. In other embodiments, the mapping may be achieved via contact sensors, certain of which may be moved relative to the surface of the heart. Any other suitable method for mapping the heart and/or obtaining the image **191** is contemplated. In some arrangements, rapid collection of high density electrograms from the left and right atria is possible. Sorting or ranking algorithms can be used on the electrograms, such as discussed above. Signals can be assessed based on stability—for example, non-stable electrograms may be omitted or discounted, whereas stable electrograms (e.g., those with regular atrial-beat-to-atrial-beat [“A-A”] intervals) may be compared. Local A-A intervals may be assessed and compared. One or more targets may be identified for ablation based on the most rapid (highest frequency) stable signal or signals.

As can be appreciated from FIG. **11**, in some embodiments, multiple AF drivers can be identified simultaneously. For example, the algorithms used to analyze and rank, sort, characterize, weight, or otherwise assign value to waveforms can do so in a way that accounts for the possibility that multiple drivers may be present. In FIG. **11**, four potential driver positions **192p**, **193p**, **194p**, **195p** have been identified.

FIG. **12** is a schematic representation illustrating an atrial driver isolation procedure to electrically isolate three of the actual atrial drivers **193a**, **194a**, **195a**, which are representatively shown in FIG. **11**, so as to prevent undesired signals from these drivers from propagating along the atrial wall. Ablation paths **120**, **122** may be similar to those shown in FIG. **2**. For example, standard PVI procedures may be employed. The actual driver **192a**, however, can be addressed in a manner different from what is shown with respect to the driver **131** in FIG. **4**. For example, in many instances of prior art techniques, the additional paths **140**, **142** and/or **144** of FIG. **4** may be formed in other procedures because an exact location of the drivers **131**, **132**, **133**, **134**, **135**, **136**, **137** and/or **138** could not be determined. However, by determining the exact or approximate position of the actual driver **192a**, focal ablation at, on, or near the driver **192a** is possible, as shown in FIG. **13**.

FIG. **13** is a schematic representation illustrating an atrial driver isolation procedure to electrically isolate two of the atrial drivers **194a**, **195a** shown in FIG. **11** in a manner slightly different than that shown in FIG. **12**, and further showing a focal ablation procedure to locally isolate the atrial driver **192a** (of FIG. **12**). In FIG. **13**, the atrial path **120** is the same as shown in FIG. **12**. However, a different ablation path **123** may be formed to isolate the drivers **194a**, **195a**. The path **123** may be smaller (or larger) than the path **122** and more focused, or informed, to ensure that the drivers **194a**, **195a** are isolated within the PVI ablation path. This can reduce the amount of scarring of the heart wall. The

focal ablation **125** can also result in much less damage to the heart than would be possible if the location of the driver **192a** were unknown. As can be appreciated from FIG. **13**, electrical isolation of the driver **192a** via ablation can in some instances involve direct ablation of the driver itself, rather than encircling the driver with scar tissue.

FIGS. **14A-14C** are flowcharts depicting illustrative methods **200**, **240**, **260** of treating atrial fibrillation. Some of the stages shown in each chart may be performed by a practitioner; others may be performed via devices and/or systems described herein. For example, in some instances, at least some of the steps may be performed via a computing device. In still further embodiments, at least some of the steps may be automated. Accordingly, any suitable subset of the stages shown in any of FIGS. **14A-14C** can stand alone as a separate or independent method. Moreover, any suitable order of the depicted stages is contemplated.

With reference to FIG. **14A**, the method **200** includes a stage **202** at which at least a portion of the heart is mapped to determine the electrical isolation of one or more pulmonary veins. At decision block **204**, it is determined from the mapping whether the one or more pulmonary veins are electrically isolated from the atrium wall. If not, then the method proceeds to stage **206** at which the pulmonary veins are isolated from the atrium wall via ablation. If they are isolated, then the method proceeds to stage **208**. At stage **208**, multiple trace electrograms of the atrium wall are generated using a sensor, or stated otherwise, via any suitable sensor system. Examples of suitable sensor systems are discussed above with respect to FIG. **9**, and further examples are discussed below with respect to FIGS. **15-26**, **39**, **40**, and **43**. In many embodiments, the sensor system is positioned within the heart of the patient to obtain the data used in the electrograms, although other or further sensor systems may employ detection devices that are situated at an exterior of the patient. At stage **210**, the electrogram traces are ranked according to their uniformity (regularity, lack of complexity, etc.) and/or their frequency. As a result of stage **210**, the position(s) on the heart that are associated with the highest ranking electrogram trace(s) can be identified. These identified positions are the target sites at which drivers are likely to be (or be near). In other or further methods, the ranking can be based on other or further criteria, such as previously discussed. The identification may include tagging, marking, coloring, or otherwise altering an image of the heart, such as the image **191** discussed above.

At stage **212**, focal ablation is performed at a target site, or ablation lines are created to isolate the target site associated with an atrial driver. At decision block **214**, it is determined whether atrial fibrillation has changed with the treatment thus far. If not (or if it has changed, but there are still atrial fibrillation issues), then the procedure loops back to stage **212**. If so, then the procedure proceeds to decision block **218**, at which it is determined whether atrial fibrillation has been fully resolved. If not, then the procedure proceeds to decision block **220** at which it is determined whether a remapping event should take place. If not, then the procedure loops back to stage **216**. If so, then the procedure loops back to stage **208**. If the atrial fibrillation has been fully resolved, then the procedure is at an end.

FIG. **14B** is a flowchart depicting another illustrative method **240** of treating atrial fibrillation. The method **240** closely resembles the method **200**. However, the stages **202**, **206**, and the decision block **204** are omitted. Accordingly, the method **240** proceeds without isolating the pulmonary veins and/or verifying that the pulmonary veins are electrically isolated. In some instances, the method **240** can

successfully resolve AF without isolating the pulmonary veins. The method **240** can identify and electrically isolate only the drivers that are the source of the AF. Otherwise, the stages and decision blocks **208**, **210**, **212**, **214**, **216**, **218** of the method **240** can proceed in the same manner as discussed above with respect to the method **200**.

FIG. **14C** is a flowchart depicting another illustrative method **260** of treating atrial fibrillation. At stage **208**, multiple trace electrograms of the atrium wall are generated using a sensor (or sensor system—e.g., any suitable sensor system, such as those discussed above and below). At stage **262**, each electrogram is mapped to a physical location on the atrium wall, such as by generating or modeling a 3-D representation of the atrium wall. Each electrogram may be associated with specific locations on a model or image of the atrium wall thus generated. At stage **210**, the electrogram traces are ranked according to their uniformity (regularity/lack of complexity/etc.) and/or their frequency. As a result of stage **210**, the position(s) on the heart that are associated with the highest ranking electrogram trace(s) can be identified. These identified positions are the target sites at which drivers are likely to be (or be near). In other or further methods, the ranking can be based on other or further criteria, such as previously discussed. In some embodiments, a representation of some property of the electrogram is assigned to the 3-D model. For example, each electrogram may be represented by a color, grayscale shade, or other suitable visual indicator corresponding with a property of the electrogram, such as its frequency, stability, and/or uniformity, or its ranking or weighting as a potential driver location (which may be calculated or evaluated in any suitable manner, such as discussed above). Stage **210** can include overlaying the 3-D map with a representation of a fourth dimension. At stage **264**, an ablation treatment is planned to electrically isolate the target sites. The ablation treatment may include directly ablating and/or encircling with ablated tissue one or more of the atrial drivers.

In some instances, stage **264** may be omitted, or it may be automatic. For example, in some embodiments, the ranking at stage **210** may include assigning various threshold values to potential ablation sites. For example, a likelihood that a position on the atrium wall is at or near a driver may be assigned a color. At stage **210**, two or more, three or more, or four or more colors may be used to rank various positions on the atrium wall within a like number of probability ranges. For example, three colors may be used to identify highly likely, moderately likely, or unlikely driver positions (e.g., yellow, blue, red, respectively). In certain of such procedures, the stage **264** may be omitted, or it may be automatic. For example, the ablation treatment plan at stage **264** may merely be to perform focal ablation at each position that is marked in the “highly likely” color (e.g., yellow).

At stage **266**, the sensor is removed from the patient. At stage **268**, the ablation is performed.

FIGS. **15-22** illustrate a non-limiting embodiment of a system **305**, and non-limiting embodiments of components thereof, that can be used in, with, or as one or more of the methods and systems previously discussed. The system **305** can include a non-contacting sensor array that is configured to be positioned within the heart and to obtain measurements at positions that are spaced from the wall the heart.

FIG. **15** is a schematic diagram of the system **305**, which can be used identifying one or more atrial drivers. The system **305** may be referred to as an electrophysiology mapping system. In some embodiments, the system **305** may comprise the EnSite® system available from St. Jude Medical of St. Paul, Minn. In some embodiments, the EnSite®

system presents electrophysiologic data on a static geometry of the heart, and it should be recognized that certain heart information (e.g., EP activation) is available on a single beat basis. Further examples of systems that may be used are provided in U.S. Pat. Nos. 6,978,168; 7,187,973; and 7,189,208, the entire contents of which are hereby incorporated by reference herein. Certain of these patents provide details for receiving cardiac signals (e.g., electrogram) that represent electrical signal transmission along the cardiac wall. Stated otherwise, details are provided for mapping multiple points of electrogram data to physical regions on the cardiac substrate, which can be accomplished via sensors such as described below.

In the illustrated system **305**, a patient **310** is undergoing a minimally invasive ablation procedure. The initial stages of the procedure involve mapping the heart and obtaining trace electrograms, as described hereafter. A specialized catheter **314**, which in some arrangements may be a branded EnSite Array™ catheter, is coupled to a breakout box **312**. A conventional electrophysiology catheter **316** may also be introduced into the patient while a variety of surface electrodes **311** are used to monitor cardiac activity during the procedure. The breakout box **312** permits the ECG cables and EP system to be coupled to additional hardware, which is not shown in this figure. The patient interface unit **318** couples the catheter **314** to a workstation computer **320** and its related peripherals. The workstation operates under the control of a software program, which provides a substantial amount of information to the attending physician.

In use, the physician will see a map image similar to that shown in FIG. **19** on a monitor **323**. A computed index **351** may also be shown to the physician as indicated by index value “0.93” seen on the monitor **323**, although in other instances the computed index **351** may not be shown. In other or further instances, trace electrograms may be shown on the monitor **323** (such as depicted in FIG. **24**). In general, the physician is able to visualize the intracardiac cavity **332** containing the catheter **314**, as seen in FIG. **19**, on the monitor **323**, which may be in color. Color can be used to reduce the clutter in the image. Expressed or displayed on this wire frame geometry image **350** are maps and other electrophysiology information derived from the catheter **314**. In some procedures, a patient is also provided with one or more pacing catheters **324** which are coupled to a temporary pacer **326** through the breakout box **312**. The temporary pacer **326** allows the physician to make measurements while varying the A-V delay and the V-V delay time. Pacing rate may be varied to ensure capture.

Turning to FIG. **16**, the heart **330** is shown schematically with a right ventricle **332** containing the catheter **314** and a conventional EP catheter **316** as well as the pacemaker lead **324**. In brief, software running on the workstation **320** in FIG. **15** can create an electrophysiological map of the heart during a single heartbeat as follows. In operation current sourced from a pair of electrodes (electrode **340** and **342**) and injected into the heart chamber **332**. A roving catheter, shown as EP catheter **316**, is located on the endocardial surface **331** toward the exterior of the heart this catheter may be moved widely and may be placed on the interior heart surface along the septum is shown by reference numeral **333**. The injected current is detected through the electrode **344** on the EP catheter **316**. This location is determined and as the catheter is moved about the chamber, complete chamber geometry can be built up by noting the sequential positions of the electrode **344**. Incorporated references describe this process in more detail, but for purposes of this disclosure, a convex hull modeling technique is used to build

a statically displayed interior geometry of the heart chamber by selecting certain locations developed from the electrode motion. The convex hull model of the interior chamber of the heart can be smoothed and a representative wire grid displayed to the physician. Such a wire grid is shown in FIG. 19 as element 350.

The catheter 314 also carries an array of passive electrode sites, which may also be referred to a sensors, typified by electrode site 346. These electrodes are arrayed around the geometric access of the balloon 347. At any given instant some of these electrode sites are pointed toward the exterior surface wall 331 and the septal wall 333. By computing the inverse solution, the electrophysiologic potentials passing along these surfaces can be measured within one beat. Reference may be had to U.S. Pat. Nos. 5,297,549; 5,311,866; 6,240,307 and 5,553,611 for further discussion of the inverse solution and the creation of the electrophysiologic map. Each of these references is incorporated in its entirety in the present application.

In some systems, the depolarization wavefront is displayed on a representative geometric surface such as the grid surface 350 of FIG. 19. The workstation 320 animates this electrophysiology data and the propagation of the electrical wavefront along the interior surfaces of the heart can be monitored. Wavefronts 380, 382, and 383 are sequence movements of the stimulus from pacing site 384 seen in FIG. 19.

FIG. 20 shows an equivalent circuit implementation to facilitate a description of conduction volumetry measurements made from a catheter 314. Returning to the geometry of the array on the catheter 314 the interior of the balloon 347 is non-conductive which provides a limited field of view for each of the electrode sites on the surface of the balloon. In essence each electrode responds only to electrical activity bounded by the heart wall, which is directly opposite the electrode site. For example, an electrode such as electrode 346 sees electrical activity and conductance data bounded by the wall 331 and is blind to electrical activity on wall 333. In a similar fashion, an electrode such as electrode 350 sees only electrical activity occurring on wall surface 333. By monitoring the voltages on the array electrodes during the pulse, or more particularly measuring the resistance between adjacent columnar pairs of electrodes as indicated by exemplary difference amplifier 386 it is possible to compute the volume of a partial slice 388 of the chamber volume best seen in FIG. 21. It is important to note that the volume measurement is segmented into several local volumes typified by volume 388.

FIG. 21 shows a slice of chamber volume computed by measuring the difference in resistance between electrodes adjacent along the axis 321. This view shows that the volume segments are non-overlapping and extend along the axis 321. The conductance term R is the resistance measured at electrodes in the passive array. This value is directly available to the software in the program, and Rho is the conductance of the blood in ohms-centimeters. D represents the distance between adjacent electrode sites in the passive array along the axis 321. This value is known from the geometry of the catheter 314. The preferred conduction volumetry algorithms can be computed very fast and the volume changes throughout a single beat of the heart may be tracked. The measurement of chamber volume is most accurate at the mid volume level indicated in FIG. 20 at reference 390. It is preferred but not required to sum or stack the independent volume measurements to create "columnar values" centered on the axis 321. This is achieved by adding volumes 392 through 396 to create a column volume 390

located near the septum. A similar process is repeated to create a column volume near the wall 331 as shown as a slice 388 in FIG. 21 as well as elsewhere around the chamber.

Without being bound by theory, it is believed that the most effective heartbeat will involve the simultaneous and progressive activation of all of the muscle tissue, which should result in a self similar reduction in the measured volume among all of the volume segments measured.

FIG. 22 is a display of four representative volume segments of the heart chamber displayed as a function of time. Eight volumes may be used effectively in some arrangements. Segment 388 may correspond to the antero-lateral volume while the other traces represent other volumes such as the septal; antero-septal; anterior; antero-lateral; lateral or other volumes defined around axis 321. A suitable way to compare the self-similarity of the volume waveforms is to cross correlate them statistically. By cross correlation of the values of the segment volumes over time one can compute a number that represents the similarity relationship of the various waveforms to each other.

The system 305 may be used for generating trace electrograms. For example, in some embodiments the system 305 is not used in placement of a pacing lead, but rather is used primarily to generate data that is used in identifying atrial drivers. For example, in some embodiments, the contraction efficiency is not calculated or otherwise determined over the course of a procedure.

As shown in FIGS. 16-19, the catheter 314 may be used in mapping the right and left atria. As shown in FIG. 23, the catheter 14 is inserted into the left atrium 102, and the balloon 347 and sensors 346 are deployed. The sensors 346 are capable of obtaining information from which trace electrograms can be generated. For example, the trace electrograms shown in FIG. 24 can correspond with the positions 411, 412, 413, 414, 415, 416, 417, 418, 419 on the atrial wall shown in FIG. 23. These trace electrograms can be used in manners such as described above.

FIG. 25A is a schematic cross-sectional view of a portion of another embodiment of a system for identifying one or more atrial drivers, wherein the system includes a multi-sensor array 450 that is shown in a constricted or non-deployed state within the left atrium 102.

FIG. 25B is another schematic cross-sectional view of the portion of the system shown in FIG. 25A, wherein the multi-sensor array 450 is in an expanded or deployed state such that sensors 452 thereof are in contact with the atrial wall. Each sensor 452 may be configured to detect electrical properties of the atrial wall, from which a trace electrogram can be generated. Accordingly, a trace electrogram can be generated for each portion of the wall that a sensor 452 contacts. Further algorithms may be possible for generating trace electrograms associated with positions of the atrial wall that are between the sensors 452. Any of the foregoing electrograms thus generated can be employed in any of the methods described above.

FIG. 26 is a schematic cross-sectional view of a portion of another embodiment of a system 470 for identifying one or more atrial drivers. The system 470 includes a sensor system 472, which includes a plurality of sensor devices 474 that are positioned at an exterior of the patient 310. In particular, in the illustrated embodiment, the sensor devices 474 are skin electrodes. Any suitable number and/or arrangement of skin electrodes may be used, and these may be situated in an array. The sensor system 472 can further include, or be coupled with, a processor 476, which can store and/or process data received from the sensor devices 474. Information received from the sensor devices 474 can be

used in any suitable manner to generate trace electrograms associated with positions of the atrial wall of the heart **330**. For example, suitable methods for obtaining trace electrograms associated with the heart, based on information from the surface of the body (e.g., from body surface mapping), are disclosed in U.S. Pat. Nos. 7,016,719 and 7,983,743, the entire contents of which are hereby incorporated by reference herein. Schematic diagrams and flow charts associated with some suitable methods, which are discussed in U.S. Pat. No. 7,983,743, are provided in FIGS. 27A-27D. In some embodiments, a geometry determining device, such as a CT scanner, is used to determine the geometry of the heart **330** and/or the patient's torso. This information can be combined with the electrical signal information obtained via the sensor system **472** to map the atrial wall of the heart **330**, as well as obtain trace electrograms. The electrograms thus obtained can be employed in any of the methods described above.

It will be understood by those having skill in the art that changes may be made to the details of the above-described embodiments without departing from the underlying principles presented herein. For example, any suitable combination of various embodiments, or the features thereof, is contemplated.

FIG. 28 is a schematic representation of an illustrative method by which a non-contact sensor collects cardiac signals from multiple regions of the cardiac substrate or atrial wall. In particular, a non-contact sensing system in which a sensor array is inserted within a chamber of the heart but does not contact the wall of the heart, such as the system depicted in and described with respect to FIGS. 15-24, can be used in the method. A portion of the atrial wall **650** is shown. The sensor array (e.g., the balloon or basket with multiple sensors, such as that used in the EnSite® array) can project potentials to the atrial wall **650** in a manner such as shown in FIG. 21. Each sensor may project the potentials over an area **671**, **672**, **673**, **674** of the atrial wall **650**, such that each area **671**, **672**, **673**, **674** represents a sensed wall region. A center point of each projected potential is shown at the diamonds **661**, **662**, **663**, **664**, which may also be referred to as the projected potentials. As can be seen in FIG. 28, the projected potentials may overlap one another. The sensor potentials can be the average of the wall potential sensed through a blood volume, such as depicted in FIG. 21.

The projected potentials can be used to estimate the actual potentials at the atrial wall **650**. Various positions at which potential estimations may be provided are depicted as hexagons, such as the estimated potential regions **681**, **682**, **683**, etc. For each position, the estimated potential may be obtained by interpolating the projected potentials **671**, **672**, **673**, **674**.

Electrocardiograms of the wall region **650** may be obtained from the interpolated or estimated potentials **681**, **682**, **683**, etc. The electrocardiograms may be evaluated, processed, manipulated, or used in any suitable manner to identify a location of a driver **630**. Methods for using such electrocardiograms to identify the positions of the drivers **630** are discussed above (e.g., in FIGS. 14A-14C) and below. Following is the discussion of another method for identifying the position of a driver **630** and treating AF.

FIG. 29 is a flowchart depicting a method of treating AF. At stage **702**, potentials of the wall region **650** are measured and collected over a period of time (e.g., in the form of one or more electrocardiograms). The measurements may be made via a plurality of sensors that extend in at least two dimensions. For example, as shown in FIG. 21, the illus-

trated sensor array can include four sensors that are coplanar. In some embodiments, the sensors may extend in three dimensions.

At stage **704**, potentials are projected onto the wall **650**. The wall **650** may be spatially mapped. At stage **706**, potentials at a plurality of chamber wall regions (e.g., the regions **681**, **682**, **683**) are estimated by interpolating projected potentials. At stage **708**, electrograms are estimated at the plurality of chamber wall regions. At stage **710**, the estimated electrograms are ranked to identify target sites of atrial drivers. Suitable ranking algorithms are discussed above, and can include weighting of the electrograms based on their uniformity and/or frequency. Other ranking factors may include amplitude, wave shape, etc. The target sites thus identified may subsequently be targeted and ablated (e.g., focal ablation).

FIG. 30 is a plot **800** depicting an electrocardiogram of a patient who has a normal sinus rhythm and a simplified representation of the electrocardiogram. In particular, the upper curve **802** depicts a trace electrocardiogram that may be obtained in any suitable manner, including any of the various methodologies disclosed herein, whether by non-contact or contact sensors within the heart or other sensors outside of the heart (e.g., at the skin of a patient). In some embodiments, sensors such as described above with respect to **23**, **25A**, **25B**, and **26** may be used. In other or further embodiments, sensors such as described below with respect to FIGS. **39**, **40**, and **43** may be used.

The lower curve **804** depicts a simplified version of the electrocardiogram, wherein only the major voltage peaks are represented. Such simplified versions of waveforms will be used in additional plots hereafter. Accordingly, it should be understood that in many instances, although plots merely showing discrete peaks may be illustrated in some of the drawings, the plots in fact have more complicated waveforms when measured by any of a variety of types of sensing equipment.

FIG. 31 is a plot **850** depicting an electrocardiogram of a sinus rhythm with intermittent suppression by a repetitive slow atrial driver. The upper curve **852** shows the voltage readout as a function of time as it may actually be perceived by a sensor, whereas the lower curve **854** is a simplified version of the electrocardiogram in which only the major voltage peaks are represented, such as discussed above.

FIG. 32A is a schematic representation of a portion of a cardiac substrate **950**, or atrium wall, having a primary atrial driver **931** that generates a regular series of wavefronts **951**, **952**, **953**, **954**, **955**, **956** of electrical impulses that propagate toward a secondary atrial driver **932**, which may also be referred to as a bystander driver that is suppressed. The secondary driver **932** may be suppressed by dominant signals received from the primary driver **931** in the same way that occasional primary driver signals may be suppressed by neighboring drivers (which is discussed below with respect to FIGS. 34A and 34B). The secondary driver **932** is depicted in FIG. 32A as not generating any wavefronts that propagate toward the primary driver **931** due to suppression from the primary driver **931**. The primary driver **931** can be a rapid, repetitive focal point or focal region of the cardiac substrate that initiates the electrical wavefronts. Without being limited by theory, primary drivers **931** may be found at or embodied in pulmonary veins, extra pulmonary veins, ectopic sites, scar borders, ganglions, and/or anatomic boundaries.

Any suitable sensor or sensor array may be used to detect electrical signals at the region **980**, which is depicted as a hexagon, although the detection region need not in actuality

be hexagonal. In FIG. 32A, the region 980 is concentric with the primary driver 931 for ease in the present discussion. Similar concentric arrangements are also disclosed in subsequent drawings. Accordingly, a sensor may be positioned to detect a wavefront as it is generated or soon after it is generated. Such an arrangement can simplify the present discussion and analysis. However, it should be understood that in various methods of detecting drivers, the sensors may be positioned at a distance from the drivers, but algorithms such as discussed herein can be used to locate the driver based on information gathered from multiple sensors. Accordingly, some sensors that can obtain electrical data from multiple portions of the atrial wall simultaneously can be useful in identifying the location of drivers.

FIG. 32B is a schematic plot 990 illustrating the electrical signals (point-based assessment of an electrical wave), or waveforms, detected at the region 980 of the cardiac substrate. The signals wavefronts 951, 952, 953, 954, 955, 956 are represented as discrete pulses of voltage. In the illustrated embodiment, the wavefronts 951, 952, 953, 954, 955, 956 have a predictable, repeated period and a consistent amplitude. The presence of the primary driver 931 at or near the region 980 could be readily determined from a plot such as the plot 990. For example, in a method of treating AF, such as those described above and below, the electrogram associated with the plot 990 could be evaluated relative to electrograms obtained from neighboring regions to determine that the region 980 is at or near a driver (i.e., the driver 931). The regularity, frequency, and/or other properties of the wavefronts 951, 952, 953, 954, 955, 956, as compared with the same properties of wavefronts obtained from neighboring regions, can be used in identifying the region 980 as a likely candidate for the location of a primary driver.

FIG. 33A is a schematic representation of another portion of a cardiac substrate 1050 having a primary atrial driver 1031 that generates a regular series of wavefronts 1051, 1052, 1053, 1054, 1055 of electrical impulses that propagate toward a secondary atrial driver 1032. In the illustrated arrangement, the secondary atrial driver 1032 is stable and likewise generates a regular series of wavefronts 1071, 1072, 1073 of electrical impulses that propagate toward the primary atrial driver 1031. In the illustrated embodiment, the secondary driver 1032 is oriented near a boundary 1060, such as an anatomical boundary, damaged tissue, non-conducting cardiac tissue, and/or a scar. In this scenario, both drivers 1031, 1032 persist due to the boundary 1060. That is, the boundary 1060 does not allow the more rapidly firing primary driver 1031 to suppress the slower secondary driver 1032. Accordingly, although a frequency of the wavefronts produced by the secondary atrial driver is lower than a frequency of the wavefronts produced by the primary atrial driver, the boundary 1060 between the two drivers 1031, 1032 allows the secondary driver 1032 to not be suppressed by the wavefronts 1051, 1052, 1053, 1054, 1055 and thus generate its own wavefronts 1071, 1072, 1073. In other scenarios, the distance between the primary driver 1031 and secondary driver 1032, the organization of the propagating waves initiated by the secondary driver 1032, and/or the frequency and amplitude of the secondary wavefronts may prevent the secondary wavefronts from suppressing the primary driver 1031.

FIG. 33B is a schematic plot 1090 illustrating the electrical signals (e.g., waveforms) detected at a region 1080 of the cardiac substrate 1050 designated by a hexagon in FIG. 33A. The plot 1090 illustrates that the signals generated by each of the primary and secondary drivers 1031, 1032 are regular and have a predictable, repeated period. Moreover,

neither set of waveforms 1051, 1052, 1053, 1054, 1055; 1071, 1072, 1073 produced by either driver suppresses operation of the other driver 1032, 1031.

FIG. 34A is a schematic representation of another portion of a cardiac substrate 1150 having a primary atrial driver 1131 that generates a regular series of wavefronts 1152, 1153, 1154, 1156, 1157 of electrical impulses that propagate toward a secondary atrial driver 1132. The secondary atrial driver 1132 is stable and likewise generates a regular series of wavefronts 1171, 1172, 1173, 1174, 1175, 1176 of electrical impulses that propagate toward the primary atrial driver 1131. A frequency of the wavefronts produced by the secondary atrial driver 1132 is lower than a frequency of the wavefronts produced by the primary atrial driver 1131. Certain electrical wavefronts of the secondary driver 1132 can occasionally suppress wavefront generation by the primary driver 1131, typically at predictable intervals. In particular, in the illustrated embodiment, every third wavefront produced by the secondary atrial driver 1132 suppresses what would be every fourth wavefront (i.e., 1151, 1155) of the primary driver 1131. In this scenario, there is irregularity of the rapid primary driver 1131 due to intermittent suppression from the secondary driver 1132 at a lower frequency that penetrates the primary driver 1131 due to penetration of the secondary wavefronts into the region of the primary driver 1131 at times shortly after electrical tissue recovery in the region of the primary driver 1131.

Without being limited by theory, suppression, such as just discussed, is a natural phenomenon of cardiac tissue. The tissue can conduct an electrical signal, but then it is transiently dormant while it acquires an inward charge. Accordingly, in situations such as described above with respect to FIG. 34A, whether an electrical signal from the primary driver 1131 or from the secondary driver 1132 will be propagated by the cardiac tissue in the region of the primary driver 1131 can result from whichever waveform hits that region first. Typically, a fast primary driver 1131 will send signals out so quickly that it will suppress all tissue around it. However, in some instances, if the primary driver 1131 does not generate wavefronts quickly enough, another neighboring region can be released from its dormant state and conduct its own electrical signal. If that region starts a wavefront and it reaches the first region just as the first region recovers and begins the process of starting its own wavefront, the first region (e.g., the region of the primary driver 1131) will be suppressed before it can activate its own wavefront. Wavefronts from neighboring, regular drivers can have the same suppressive effects.

For slow drivers, suppression can be common. For example, for some drivers, the sinus node/pacemaker cells may only initiate an impulse every approximately 0.6 to 1.0 seconds, on average. Since cardiac tissue generally recovers within about 150 to about 200 milliseconds, any beat that begins at about 210 to about 600 milliseconds after the sinus beat will get into the sinus node and suppress it so it does not give off the next beat. This phenomenon is depicted in FIG. 31.

In the context of abnormal tissues, driver regions that generate or conduct impulses at high frequencies (e.g., with a period of less than about 150 milliseconds) may be difficult to suppress, even transiently. Without being bound by theory, this is a reason that certain methods of treating AF discussed herein (e.g., the methods in FIGS. 14A-14C) can include steps, stages, and/or algorithms for identifying drivers by regions that have a dominant and/or rapid signal frequency (e.g., algorithms in which uniformity and/or frequency value are weighted, with higher uniformity and

higher frequencies indicating stronger likelihood of driver presence). Given that the heart has anatomic boundaries, random triggers that try to send off their own signals at different frequencies, and varied distances between drivers, in some instances, signals from a dominant driver may occasionally be suppressed. Accordingly, additional methods of treating AF can include more or different steps, stages, and/or algorithms for identifying dominant drivers where occasional suppression is present.

FIG. 34B is a schematic plot 1190 illustrating the electrical signals (e.g., waveforms) detected at a region 1180 of the cardiac substrate 1150 designated by a hexagon in FIG. 34A. The plot 1190 demonstrates the periodic suppression of primary wavefronts due to activity of the stable secondary driver. For example, where wavefronts 1151, 1155 from the primary driver 1131 would be expected, only smaller wavefronts from the secondary driver 1132 are present. As discussed further below, certain methods for identifying primary or dominant drivers can take into account such occasional wavefront suppression.

FIG. 35A is a schematic representation of another portion of a cardiac substrate 1250 having a primary atrial driver 1231 that generates a regular series of wavefronts 1252, 1253, 1254, 1256 of electrical impulses that propagate toward a secondary atrial driver 1232. The secondary atrial driver 1232 functions intermittently, and thus the two operational modes of the secondary driver are designated by alternative scenarios (as indicated by the recitation "OR"). In the first or upper alternative, the secondary atrial driver 1232 is dormant, and thus the primary atrial driver 1231 is permitted to generate its electrical wavefronts at a persistent regular frequency. In the second or lower alternative, however, the secondary atrial driver 1232 is temporarily active and generates irregular wavefronts 1271, 1272 that temporarily suppress generation of a wavefront by the primary driver 1231. This intermittent suppression is depicted in the upper alternative by intermittent broken lines where wavefronts 1251, 1255 would be expected. Also, the secondary driver 1232 may be temporarily suppressed by incoming wavefronts initiated by the primary driver 1231 causing the initiation of wavefronts from the secondary driver to be muted. If a period of time between wavefronts initiated by the primary driver occurs, the secondary driver may initiate a wavefront towards the primary driver 1231.

FIG. 35B is a schematic plot illustrating the electrical signals (e.g., waveforms) detected at a region 1280 of the cardiac substrate 1250 designated by a hexagon in FIG. 35A. The periodic suppression of the primary wavefronts 1251, 1255 due to activity of the intermittent secondary driver 1232 is indicated by occasional signals that vary in strength and/or time (e.g., the signals may be slightly earlier than would otherwise be expected, which may result in suppression) from the otherwise regular pattern of signals from the primary driver 1231.

FIG. 36 is a schematic illustration of a portion of a method 1300 for identifying multiple drivers from a trace electrocardiogram. The method 1300 can include obtaining the trace electrocardiogram 1305 in any suitable manner, which is depicted at stage 1310. The electrocardiogram 1305 may be obtained, for example, via any of the sensors and sensor systems described herein, including contact sensors, non-contact sensors, and/or sensors positioned at an exterior of a patient. At stage 1320, unique frequencies from the electrocardiogram 1305 are isolated and dominant drivers are identified. Although these activities are depicted as occurring in a single step in FIG. 36, in some embodiments, the isolation of unique frequencies and the identification of

dominant drivers may be carried out in distinct steps. Isolation of the dominant frequencies may be performed in any suitable manner, such as, for example, via a Fourier transform and/or any other suitable algorithm. Identification of dominant drivers may involve identifying a specific region on a three-dimensional map of the heart that is responsible for a dominant frequency. Mapping of the heart and correlation of a signal source to a specific region of the resultant map may be performed in any suitable manner, such as, for example, any methodology discussed above. One or more portions of the isolation and/or identification steps may be performed via a computer or computer program. FIG. 36 includes a schematic plot 1330, which may be a byproduct of and/or an intermediate result of stage 1320. In particular, the plot 1330 shows provides a visual representation of two unique frequencies, depicted as an upper segment 1332 and a lower segment 1334, that have been isolated from the electrocardiogram 1305. In some instances, the upper segment 1334, with its higher frequency and greater amplitude, may be identified as (or identified as being associated with or being at or near) a primary driver.

FIG. 37 is a schematic representation of another portion of a cardiac substrate 1450 having an atrial driver 1433 that is spaced from a series of five different sensors 1481, 1482, 1483, 1484, 1485 (or sensed regions, such as the regions 681, 682, 683 in FIG. 28) by varying amounts. Each sensor or sensed region is schematically represented by a numbered hexagon, although the region sensed may not, in fact, be hexagonal. Moreover, it may be desirable merely to sense at various distances from the driver 1433, and not necessarily in a straight line. The distances are represented by broken-lined concentric circles. Accordingly, although in the illustrated arrangement, the sensors 1481, 1482, 1483, 1484, 1485 are arranged in a straight line, the signals sensed thereby that originate at the driver 1433 will generally be the same at any point along the circle associated with that sensor. However, signals that originate at positions that are spaced from the driver 1433 will appear at different times along each circle. As can be appreciated from the foregoing, in order to locate an atrial driver 1433, particularly where the position of the atrial driver 1433 is not known from the outset, it can be advantageous to have sensors so as to cover a multi-dimensional surface of the wall 1450, rather than merely a one-dimensional line along the wall 1450. For example, a series of sensors may desirably be placed on the wall in two dimensions, such that they cover an area when viewed in a plan view. In further embodiments, the sensors may further follow a three-dimensional contour of the wall 1450. Non-contact sensors such as described above can obtain measurements in three-dimensions in this manner. Contact sensors such as shown in FIGS. 25A and 25B may also provide such three-dimensional data. Additional contact sensors that are suitable for obtaining such measurements are described below with respect to FIGS. 39, 40, and 43.

FIG. 38A is a schematic plot 1492 illustrating the electrical signals (e.g., waveforms) that may be detected by each of the sensors 1481, 1482, 1483, 1484, 1485 when the atrial driver 1433 is a primary driver from which wavefronts regularly propagate outwardly. For example, a signal or wavefront 1401 may first be detected by the sensor 1481, then by the sensor 1482, then by the sensor 1483, then by the sensor 1484, and finally by the sensor 1485. The wavefront 1401 thus may clearly propagate in a direction away from the driver 1433. The same is also true of a subsequently generated wavefront 1402.

FIG. 38B is a schematic plot 1494 illustrating the electrical signals (e.g., waveforms) that may be detected by each

of the sensors **1481**, **1482**, **1483**, **1484**, **1485** when the atrial driver **1433** is instead a secondary driver that has a lower frequency than a neighboring driver (e.g., a neighboring primary driver) and/or that generates wavefronts intermittently. Accordingly, the secondary driver **1433** may be subject to signal suppression, such as discussed above. Due to the secondary, or less dominant nature of the atrial driver **1433** (as may result, for example, from the driver **1433** having a lower frequency), wavefronts may generally propagate toward the secondary driver **1433**, rather than away from it. For example, in the illustrated plot **1494**, the driver **1433** may occasionally generate a wavefront, such as the wavefront **1403**. This wavefront **1403** may start to propagate outwardly from the driver **1433**, as shown by the later detection of the wavefront **1403** by the sensor **1482**. However, by the time the wavefront **1403** reaches the position of the third sensor **1483**, a different wavefront **1404** from some other source (e.g., a neighboring primary driver) may have already triggered the cardiac tissue in regions external to the circle associated with the sensor **1482**. Indeed, the wavefront **1404** was previously sensed by the sensor **1484**, and was sensed prior to that by the sensor **1485**. Accordingly, the sensors **1485**, **1484**, **1483** are shown as having detected the wavefront **1404** propagating toward the driver **1433**. The wavefront **1404** does not further trigger the cardiac tissue in the regions about the sensors **1482** and **1481** in the illustrated arrangement, however, since the wavefront **1403** has already triggered the cardiac tissue and it has not yet recovered.

Moreover, before the slower-operating driver **1433** is able to generate another wavefront of its own, it is triggered by another wavefront **1405** that originated elsewhere (e.g., at the neighboring primary driver). This wavefront **1405** is shown in the plot **1494** as propagating toward the driver **1433**, given that wavefront **1405** was first detected by the outermost sensor **1485**, and was then detected by the progressively more inwardly positioned sensors **1484**, **1483**, **1482**, and then **1481**.

In view of the foregoing, it may be said that the driver **1433** occasionally initiates wavefronts that propagate outwardly. However, wavefronts predominantly propagate inwardly toward the driver. The property of wavefronts generally propagating outwardly from primary drivers and propagating inwardly toward secondary drivers may be used in locating primary drivers, such as in the methods described below with respect to FIGS. **41** and **42**.

FIG. **39** is a plan view of an embodiment of a sensor assembly **1500** that may be useful in obtaining measurements regarding wavefront propagation, among other wavefront and/or waveform properties. The sensor assembly **1500** can include an array of sensors **1502** that extend in at least two orthogonal directions, or two dimensions (e.g., in the X- and Y-directions of the illustrated planar view). The sensors **1502** may extend in a third direction as well (e.g., in the Z-direction into/out of the page, in the illustrated view) to readily conform to a three-dimensional contour of a heart wall **1550**. Each sensor **1502** may be capable of detecting electrical potentials of a region **1580** of the heart wall **1550**. The sensors **1502** may define a multi-dimensional (2-dimensional or 3-dimensional) sensing area. In some embodiments, the sensor assembly **1500** may operate in a unipolar mode, e.g., in which each sensor **1502** detects a potential relative to a common voltage. In other or further embodiments, the sensor assembly **1500** may operate in a bipolar mode, e.g., in which potential differences between adjacent sets of sensors **1502** are detected.

In the illustrated embodiment, the sensor assembly **1500** includes a positioning catheter **1506** that can be used to

dynamically change a position of the sensor array. In some applications, the sensor **1500** is positioned on the substrate **1550** for a period of time that atrial fibrillation is observed (e.g., over multiple heart beats), and in further applications, electrogram data can be acquired simultaneously with near field and/or far field electrogram data. Methodologies, such as those disclosed above and below, can be used to identify potential atrial drivers and portions of the sensed area can be recorded or identified as potential treatment targets. The sensor **1500** may then be relocated to a new portion of the substrate **1550**. In some embodiments, the sensor assembly **1500** can provide a more detailed view of a smaller portion of the cardiac wall **1550** than may be obtained with certain embodiments of the sensor depicted in FIGS. **25A-25B**.

The sensor assembly **1500** can further include a support structure **1504**, such as a wire or narrower catheter, to which the sensors **1502** are mounted. In the illustrated embodiment, the support structure **1504** defines a single branch that is spiraled. In some embodiments, the support structure **1504** may be resiliently flexible, and may have a springing action. For example, in the illustrated embodiment, the support structure **1504** may be capable of concave or convex deformations relative to a center point of the spiral, which may aid in following a contour of the heart wall. As previously mentioned, the sensor array may be particularly useful in detecting the direction of propagation of wavefronts relative to a driver **1530**, as depicted by the broken arrows.

In some embodiments, the sensor assembly **1500** can comprise a Reflexion HD™ High Density Mapping Catheter, which is available from St. Jude Medical of Little Canada, Minn.

FIG. **40** is a plan view of another embodiment of a sensor assembly **1600** that includes multiple contact sensors **1602** that can extend along a cardiac substrate **1650** in at least two orthogonal directions, or stated otherwise, in at least two dimensions, to define at least a two-dimensional sensing area. Like the sensor assembly **1500**, the sensor assembly **1600** may also be configured to extend in three dimensions to follow a contour of the heart wall **1650**. In various embodiments, the sensor assembly **1600** may be operated in a unipolar and/or in a bipolar mode.

Each sensor **1602** of the assembly **1600** may be capable of detecting electrical potentials of a region **1680** of the heart wall **1650**. The sensors **1602** may define a multi-dimensional (2-dimensional or 3-dimensional) sensing area. In the illustrated embodiment, the sensor assembly **1600** includes a positioning catheter **1606** that can be used to dynamically change a position of the sensor array. In some embodiments, the sensor assembly **1600** can provide a more detailed view of a smaller portion of the cardiac wall **1650** than may be obtained with certain embodiments of the sensor depicted in FIGS. **25A-25B**. The sensor assembly **1600** can further include a support structure **1604**, such as one or more wires or narrower catheters, to which the sensors **1602** are mounted. In the illustrated embodiment, the support structure **1604** defines five branches that extend from a distal end of the positioning catheter **1606**. In some embodiments, the support structures **1604** may be resiliently flexible, and may have a springing action. The sensor array may be particularly useful in detecting the direction of propagation of wavefronts relative to a driver **1630**, as depicted by the broken arrows.

In some embodiments, the sensor assembly **1600** can comprise a PentaRay® NAV Catheter, which is available from Biosense Webster® of Diamond Bar, Calif.

FIG. **41** is a flowchart depicting a method of treating atrial fibrillation **1700**. The method can exploit the properties of

drivers discussed herein to aid in identifying probable or actual positions of those drivers and subsequently ablating (e.g., focal ablating) the drivers.

At stage **1702**, local electrograms are acquired from a cardiac substrate. The local electrograms may be acquired in any suitable manner, such as discussed herein. For example, in some embodiments, non-contact sensor arrays may be used. In other embodiments, sensor arrays (e.g., as provided by the sensor assemblies **1500**, **1600**) may be used.

At stage **1704**, it is determined whether any local electrograms have stable frequencies. If the determination is affirmative, the method continues on to stage **1706**, if not, the process progresses to stage **1742**.

At stage **1706**, it is determined whether the local electrogram, or a series of local electrograms (e.g., such as described above with respect to FIGS. **38A** and **38B**) show a propagation of an electrical wavefront. In particular, it is determined whether an electrical wavefront is shown predominantly propagating in a single outward direction, or outwardly from a region. If the determination is affirmative, then the process continues to stage **1708**. If, however, the determination is negative, or if the wavefronts predominantly propagate in a direction toward a given region, then the process continues to stage **1720**. The determination at stage **1706** may include comparison of different electrograms. For example, all electrograms may be compared with one another, and physical locations of the heart that are associated with each electrogram may be taken into consideration to determine in what direction an electrical wavefront propagates.

At stage **1708**, a local electrogram is identified as a probable atrial driver. Stated otherwise, a position of the heart wall that is responsible for generation of the electrogram having the properties that led to the arrival at stage **1708** is identified as a position at which a primary driver is likely to be located. For example, a three-dimensional image or model of the heart (e.g., the image **191** discussed above) may be marked with a color or other indicator to identify the potential driver.

At stage **1710**, the probable atrial driver electrograms are ranked to determine which electrogram is most likely to be associated with an atrial driver. In some ranking algorithms, an electrogram is more likely to be associated with an atrial driver if a propagating signal, or peak voltage, occurred there earlier than it did in other electrograms. Stated otherwise, in some processes, early occurrences of a propagating peak are given a greater weight in a weighting algorithm, or are otherwise assigned higher likelihood that an atrial driver is associated with the electrogram. The position of earliest occurrence can yield the most likely position of the driver, in some algorithms.

Other factors may be evaluated instead of, or in addition to, peak propagation at this stage. For example, frequency, stability, waveform shape, and/or other wave properties, such as those discussed above, may be evaluated. In some instances, the positions at which drivers are potentially located that have the highest frequencies are ranked and identified as the most best candidates for ablation.

In some instances, a further stage may occur after stage **1710** in which one or more rankings are mapped to a representation of the heart. For example, a three-dimensional image or model of the heart may be marked with a color or other indicator to identify a potential driver, or target site for ablation. If multiple drivers are identified, with one driver having a higher frequency and one or more further drivers having a lower frequency, such that the higher frequency driver may have a higher likelihood of

being a primary driver, the marking or identification may proceed in a manner to distinguish the various drivers from one another. For example, the higher frequency driver may be marked with a color or otherwise identified in a manner that signifies that the position on the heart is likely a driver and is thus a good candidate for ablation, and the one or more lower frequency positions may be identified as less likely positions at which a primary driver is located. Even where only a single potential driver is identified, a similar identification may take place. For example, in some instances, it may be determined that any potential driver having a frequency that is above a threshold value (e.g., having a period of no greater than 100 milliseconds, in some instances) is a good candidate for ablation and thus may be identified accordingly (e.g., by marking a three-dimensional map with a specific color or other indicator). Other thresholds may also be determined. For example, potential positions that exhibit periods at or below a lower threshold may be identified as good driver candidates, positions that exhibit periods between the lower threshold and an upper threshold may be identified as fair driver candidates, and positions that exhibit periods at or above the upper threshold may be identified as poor driver candidates. Other ranking values and identification systems are also contemplated.

At stage **1712**, the highest and/or higher ranked probable atrial driver electrograms are located and focal ablation is performed at one or more of the locations. The location may be determined from a map of the heart, which may be directly correlated to the various positions from which the electrograms are gathered, in manners such as discussed above.

At stage **1714**, it is determined whether atrial fibrillation has been resolved. If so, then the method is at an end at stage **1716**. If not, the method proceeds to stage **1730** to determine whether the atrial fibrillation, though not resolved, has at least changed. If there has been a change, then the method loops back to stage **1712** again. However, if there has been no change, then the method proceeds to stage **1722**. In some instances, after an evaluation is made at stage **1714**, reconsideration may be made in the setting of isopenaline (isoproterenol, or "Isuprel").

Reference is again made to stage **1720**, the completion of which also results in progression to the stage **1722**. At stage **1720**, if the decision at stage **1706** is negative, then the local electrogram is identified as a probably secondary driver. Reassessment of whether a probable secondary driver is in fact a primary driver occurs at stage **1722**. If it is determined that what was originally considered to be a secondary driver may in fact be a primary driver, then the method can loop back again to stage **1708**.

Referring again to stage **1704**, if no local electrograms demonstrate stable frequencies, then the method can proceed to stage **1742**, at which it is determined whether any local electrograms have intermittent suppression of a stable frequency, or stated otherwise, whether the electrogram would have a stable frequency, but for the existence of intermittent suppression of expected signals or wavefronts at the otherwise stable frequency. If such suppression is or appears to be present (e.g., suppression such as shown in FIG. **34B** or **35B**), then the method proceeds to stage **1744**. If not, then the method proceeds to stage **1750**, at which the electrogram substrate locations are identified as unlikely atrial driver sites. The identification can include the marking of a three-dimensional model of the heart in manners such as discussed above.

At stage **1744**, it is determined whether the local electrogram returns to the original, regular frequency after sup-

pression. If so, then the method cycles back to stage **1706**. If not, then the method cycles back to stage **1750**. After arriving at stage **1750**, a sensor may be repositioned to a new area of the heart wall (e.g., for some contact sensors), or a new sensing region may be identified (e.g., for other, larger-area contact sensors and/or non-contact sensors that sense over a large region). The method **1700** may then be repeated at the new region of the heart.

The method **1700** can be repeated as treatment progresses. For instance, as an atrial driver location is treated by ablating the cardiac tissue associated with the targeted site, newly acquired sensor data can be acquired and then used to assess the substrate for other probable atrial driver targets.

As with other methods herein, one or more of the stages may be performed by a computer or other specialized equipment. For example, any suitable program that implements algorithms such as described herein is contemplated. Moreover, any suitable subset of stages may constitute a separation method. By way of example, some methods may comprise stages **1702**, **1704**, **1706**, and **1708**; further methods may additionally comprise stage **1710**; and further methods still may additionally comprise stage **1712**. Some methods may comprise stages **1702**, **1704**, **1742**, **1744**, **1706**, **1708**, and/or **1710**; and further methods may additionally comprise stage **1712**.

FIG. **42** is a flowchart depicting another method of treating atrial fibrillation. The method closely resembles the method **1800**. In particular, the stages **1804**, **1806**, **1808**, **1810**, **1812**, **1814**, **1820**, **1822**, **1830**, **1842**, **1844**, and **1850** can be the same as the stages **1804**, **1706**, **1708**, **1710**, **1712**, **1714**, **1720**, **1722**, **1730**, **1742**, **1744**, and **1750**. However, the method further includes the stages **1803** and **1840**. Any suitable subset of the foregoing steps is also contemplated.

The step **1803** resembles the step **1702** discussed above, but further includes acquisition of near field electrograms from the substrate. The collection of the near field and local electrograms can be simultaneous or substantially simultaneous, and may be performed in any suitable manner. The term “near field electrogram” is meant in its ordinary sense.

The method proceeds from stage **1804** to stage **1840** if it is determined that no local electrograms have stable frequencies. If this is the case, then it is determined whether any near field electrograms have stable frequencies. If so, then the method proceeds to stage **1806**. If not, then the method proceeds to stage **1842**. Accordingly the stage **1840** can provide another indication that stable frequencies exist relative to a region of the heart.

Either of the methods **1700**, **1800** can be combined with other methods disclosed herein to identify and/or isolate drivers. For example, in some methods that include at least some of the stages of the methods **1700**, **1800** can further include some or all of the stage of the methods **200**, **240**, **260**, **700**. For example, ranking algorithms that weigh the frequency, regularity (or stability), etc. of electrograms, wavefronts, and/or wavefront patterns may be used before, after, or otherwise in conjunction with any suitable stage or stages of the methods **1700**, **1800**. By way of illustrative example, the stages **702**, **704**, **706**, and **708** of the method **700** may be performed in conjunction with the stages **1702**, **1803** of the methods **1700**, **1800**, and the stage **710** may be performed in conjunction with (e.g., before, after, or simultaneously with) the stage **1710**, **1810** of the methods **1700**, **1800**.

FIG. **43** is a plan view of an embodiment of a sensor assembly **2000** in the process of gathering electrograms from a portion of an atrial wall **2050**, wherein a driver **2030** is within a sensing region of the sensor assembly **2050**. The

sensor assembly **2000** can be of any suitable variety. In the illustrated embodiment, the sensor assembly **2000** includes five separate individual support structures or branches **2004** that radiate from a distal end of a catheter **2006**. In certain embodiments, the branches **2004** can be flexible so as to be able to readily move into contact with the atrial wall **2050**. Accordingly, although the branches **2004** are consistently illustrated in the drawings as being equally spaced from one another in FIG. **43** and in subsequent drawings, the branches **2004** need not necessarily assume such a symmetrical configuration, in some embodiments. For example, in some arrangements, some or all of the branches **2004** may be closer to each other and/or some or all of the branches **2004** may be spaced further apart from each other than what is depicted in the illustrative drawings. In some embodiments, the sensor assembly **2000** can be configured to detect or otherwise provide information regarding the relative orientations of the branches **2004** such that information regarding the direction in which each branch is pointed and/or the location of each sensor **2002** is known. In some embodiments, the sensor assembly **2000**, the sensor assembly **2000** can comprise a PentaRay® NAV Catheter.

Each branch **2004** of the sensor assembly can include a plurality of sensors **2002**. Only one of the sensors **2002** is identified by the reference numeral “**2002**,” but each of the sensors is identified in the drawings by its sensor number—**S1**, **S2**, **S3**, **S4**, **S5**, **S6**, **S7**, **S8**, **S9**, **S10**, **S11**, **S12**, **S13**, **S14**, **S15**, **S16**, **S17**, **S18**, **S19**, **S20**. In some instances, the sensor assembly **2000** may operate in a unipolar mode in which each of the sensors **2002** detects a potential relative to a common reference voltage. In other instances, the sensor assembly **2000** may operate in a bipolar mode in which sets of adjacent sensors **2002** measure relative potential differences between the sensors. For example, in the illustrated embodiment, when the sensor assembly is operating in the bipolar mode, potential differences between adjacent sets of sensors that are positioned along the same branch are measured. Thus, for example, potential differences between the sensors **S13** and **S14**, between **S14** and **S15**, and between **S15** and **S16** may be obtained along one branch, and each set of adjacent sensors may thus observe the electrical activity of specific regions **2081**, **2082**, **2083**, respectively, of the atrial wall **2050**.

The positioning catheter **2006** may be used to move the distal head of the sensor assembly **2000** to a desired location along the atrial wall **2050**. This is depicted by the arrow **2001**. In some procedures, the sensor assembly **2000** may be used to map and/or measure electrical activity along a large portion of the atrial wall **2050**. In some instances, a substantial portion of the atrial wall **2050** may be observed or measured during the course of a procedure.

In some procedures, the distal head of the sensor assembly **2000** may be moved to a desired position and one or more of the branches **2004** may be moved into electrical contact with the atrial wall **2050**. The sensor assembly **2000** may then be held in place for a sufficient time to take a desired set of measurements. In various instances, the sensor assembly **2000** may be held substantially stationary relative to the atrial wall for a period of up to about 200, 400, 600, or 800 milliseconds. In other instances, an observation period may be one or more seconds, or may last for up to one, two, or three heartbeats. In some instances, the sensor assembly **2000** may be held in place for up to a minute as measurements are gathered. After a desired set of data is obtained, the sensor assembly **2000** may be moved to another portion of the atrial wall **2050**.

FIG. 43 represents a situation in which a driver 2030 is within a sensing region of the sensor assembly 2000 during an observation event. The driver 2030 regularly propagates wavefronts 2051, 2052, 2053 outwardly in manners such as discussed above. Electrograms obtained by the sensors 2004

FIG. 44A is a plot 2100 that includes electrograms gathered via the sensor assembly 2000 and that also shows a base signal 2102 of the heart. The electrogram obtained via the sensors S1 and S2 is designated DD 1-2, the electrogram obtained via the sensors S2 and S3 is designated DD 2-3, and so on. In the illustrated plot, the electrograms are arranged in ascending order of the sensor number. However, as can be seen in FIG. 44A, such an ordering of the electrograms does not necessarily or always readily reveal a pattern, such as wavefront propagation. It thus may be desirable to rank, sort, rearrange, or otherwise evaluate the electrograms and obtain information that may be used to determine an approximate or exact location of the driver 2030.

In some embodiments, a program implemented by a general purpose computer or dedicated hardware may evaluate and/or rank the electrograms based on one or more properties, such as, for example, waveform unity, frequency, amplitude, shape (e.g., slope, initial direction—whether positive or negative, sharpness, number of peaks or valleys, etc.). Timing may also be a key property used in ranking or sorting the electrograms, and in some instances, earlier presence of a wavefront will receive a higher ranking.

The result of such a ranking algorithm is shown in the plot 2105 in FIG. 44B, in which the highest ranked electrogram is listed first, the next highest is listed second, and so on. Whereas in some procedures, the ranking is performed by a computer or is otherwise automated, in other procedures, the ranking may be done visually by a practitioner. In other or further instances, the ranking may involve some form of manipulation of the electrograms by a practitioner, such as by dragging and dropping or some other movement using, for example, peripheral computer controls or a touchscreen. Thus, a practitioner might also be capable of rearranging, sorting, or ranking the electrograms into the order shown in FIG. 44B.

As mentioned above, the frequency (or period) of the electrograms can factor into a ranking algorithm. For example, the shorter the period between successive wavefronts, the higher the weighting an electrogram may receive. Thus, it may be desirable for the shortest period electrograms to appear at the top of the plot 2105, which can aid in determining the location of a target portion of the atrial wall 2050 at which a primary driver is expected to be located. In the illustrated embodiment, the period t_1 between successive wavefronts is shown.

Based on the observation or calculation that wavefronts first appear in the region between the sensors S19 and S20 and then propagate away from this region, it can be determined that the target region is closest to that region of the cardiac wall 2050. In some instances, the region between S19 and S20 is treated as a sufficiently close approximation as to the location of the driver 2030. Accordingly, the procedure may identify that location as the target spot.

In other embodiments, further calculations or observations can be conducted to conclude that the target area, although close to the position between the sensors S19 and S20, is actually between the branches that include the sensors S17, S18, S19, S20 and the sensors S1, S2, S3, and S4. Thus an even closer approximation may be obtained by making the target area somewhere between the positions

between the sensors S19 and S20 and the sensors S3 and S4. Further algorithms may be used to even more accurately interpolate the position of the driver 2030. The algorithms may take into account such factors as the relative positions of the branches of the sensor assembly 2000, the relative positions of the sensors 2002, the differences in time at which wavefronts reach the respective sensor regions, etc.

In the illustrated embodiment, a single driver 2030 is identified. In some instances, signals from the driver 2030 might appear at each of the sensing regions, such that the propagation of the wavefronts will be even more apparent than what is shown in FIG. 44B. However, as can be seen in FIG. 44B, no every sensing region has received a signal from the driver 2030. This can be due to one or more of a variety of reasons, such as poor sensor contact with the atrial wall 2050, contact with an area of the wall that is non-electrically conductive (e.g., due to a prior ablation), etc.

Once a target position for the driver 2030 has been determined, this position can be identified on a map or plot (e.g., a representative image, such as the image 191 discussed above) of the heart. In some instances, the identification can be used for subsequent ablation. For example, in some instances, detection of different driver positions takes place over a period of time, and once all such desired positions have been identified, focal ablation of specific positions that have the highest ranking, or likelihood of being primary drivers, then proceeds.

The identification may be of any suitable variety. For example, as discussed above, the identification may take the form of adding color to the three-dimensional plot. In some instances, three different colors may be used to identify driver regions of fast, medium, or slow frequencies, which may correlate with high, intermediate, and low likelihood of being primary drivers. Further discussion of identification procedures are provided above. In some instances, after a desired number of such driver positions have been identified, the ablation may then proceed, and in some instances, only the most likely candidates for primary drivers are ablated. Other systems for identifying and ablating are contemplated. Additionally, in various instances, the periods for what are considered fast, medium, and slow drivers may vary, such as from patient to patient. Accordingly, in some instances, the thresholds for what is fast, medium, or slow may be set according to a relative scale, as determined by the physiology of the patient.

FIG. 45 is a plan view of the sensor assembly 2000 in the process of gathering electrograms from another portion of the atrial wall 2050, wherein two separate drivers 2230, 2231 are within a sensing region of the sensor assembly. For example, the information gathering that is taking place in FIG. 45 can occur at a later time during the identification of possible drivers and prior to a focal ablation procedure. The driver 2230 provides wavefronts (e.g., 2251, 2252, 2253) at a higher frequency than the driver 2231 provides wavefronts (e.g., 2261, 2262, 2263).

FIG. 46A is a plot 2300 that includes electrograms gathered via the sensor assembly 2000 and that also shows a base signal of the heart. Calipers (as shown by dashed vertical lines) may be provided to assist a practitioner in identifying a minimum period from among the electrograms, as well as an electrogram for which wavefronts appear first and then propagate onward to other sensed regions. In some arrangements, the calipers may be used instead of or in addition to sorting or rearranging the electrograms in the vertical dimension.

Such a sorting or ranking is shown in FIG. 46B. In the illustrated embodiments, the two drivers within the sensing

area generate unique waveforms having nearly the same period, although the driver **2230** has a shorter period. In the illustrated sorting algorithm, the electrograms associated with the driver **2230** are higher along the vertical axis than, or stated otherwise, are ranked above, the electrograms that are associated with the driver **2231**. This may result from the higher frequency of the driver **2230**.

In some instances, a sorting algorithm may take into account various properties of the waveforms to conclude that multiple drivers are being sensed. For example, the two sets of waveforms have different overall shapes. The higher frequency waveform initiates with a small dip and then a large peak, for example, whereas the lower frequency waveform initiates with a small peak and then a large dip.

The plot **2305** shows multiple interacting drivers of distinct morphology and frequency. In **DD 13-14**, **DD 14-15**, a slow repetitive driver is noted by morphology and frequency with a simultaneous much more rapid, repetitive driver that has a distinct morphology and frequency.

As with identifying individual drivers, the target locations may be estimated approximately, or may be interpolated or otherwise calculated with a higher degree of accuracy. For example, in some procedures, one or more of the regions that are at or close to the regions between the sensors **10** and **11** and between the sensors **2** and **3** may be targeted, as the separate waveforms appear to generally propagate away from these regions.

FIG. 47 is a plan view of an embodiment of the sensor assembly **2000** in the process of gathering electrograms from another portion of the atrial wall **2050**, wherein a driver **2430** is external to a sensing region of the sensor assembly. **FIG. 48A** is a plot that includes electrograms gathered via the sensor and that also shows a base signal of the heart. **FIG. 48B** is a plot that includes the electrograms from **FIG. 48A** in a sorted or rearranged format to demonstrate propagation of wavefronts from the driver.

In some embodiments, an algorithm may be used to determine that the driver **2430** is not between any of the branches of the sensor assembly **2000**. Such algorithms may utilize time delay, sensor position, and/or other properties or variables of the sensed waves to determine an approximate or estimated location of the driver **2430**. In other or further embodiments, the algorithm may provide a suggested direction for moving the distal end of the sensor assembly **2000** in order to bring the driver **2430** within the sensing area of the sensor assembly **2000** and determine more accurately the position of the driver **2430**. In some embodiments, the suggested direction may occur on a display of the mapped heart. For example, the suggested direction may be depicted by an arrow or some other indicator on a display, which a practitioner can thus visualize and respond to in order to move the sensor assembly **2000**.

FIG. 49 is a plan view of the sensor assembly **2000** in the process of gathering electrograms from another portion of the atrial wall **2050**, wherein a first driver **2630** is at an exterior of the sensing region of the sensor assembly **2000** and a second driver **2631** is within the sensing region of the sensor assembly **2000**. **FIG. 50A** is a plot that includes electrograms gathered via the sensor assembly **2000** and that also shows a base signal of the heart. **FIG. 50B** is a plot that includes the electrograms from **FIG. 50A** in a ranked or rearranged format to demonstrate propagation of wavefronts from the drivers. Ranking or sorting of the waveforms, identification of target sites, and other procedures relative to the various sensed drivers can proceed in manners such as described above, particularly with respect to **FIGS. 43-48B**.

FIG. 51 is a plan view of the sensor assembly **2000** in the process of gathering electrograms from another portion of the atrial wall **2050**, wherein two drivers **2830**, **2831** are near a sensing region of the sensor assembly, but are outside of the sensing region. **FIG. 52A** is a plot that includes electrograms gathered via the sensor and that also shows a base signal of the heart. **FIG. 52B** is a plot that includes the electrograms from **FIG. 52A** in a rearranged format to demonstrate propagation of wavefronts from the drivers. Ranking or sorting of the waveforms, identification of target sites, and other procedures relative to the various sensed drivers can proceed in manners such as described above, particularly with respect to **FIGS. 47-50B**.

FIG. 53 is a plan view of an embodiment of a sensor assembly in the process of gathering electrograms from the same portion of the atrial wall **2050** that is shown in **FIG. 51**. The atrial wall **2050** is shown after an ablative procedure has been conducted to cease activity of the driver **2831**. **FIG. 54A** is a plot that includes electrograms gathered via the sensor and that also shows a base signal of the heart. **FIG. 54B** is a plot that includes the electrograms from **FIG. 54A** in a rearranged format to demonstrate propagation of wavefronts from the driver **2830**. Due to the continued presence of a driver, a further ablative procedure may be desired. It is noted that the driver **2831** shown in **FIG. 51** had a lower frequency than the driver **2830**, although their frequencies were about the same. As discussed above, however, in many instances, the drivers with the higher or highest frequencies will be ablated in a preliminary ablation procedure.

Any methods disclosed herein comprise one or more steps or actions for performing the described method. The method steps and/or actions may be interchanged with one another. In other words, unless a specific order of steps or actions is required for proper operation of the embodiment, the order and/or use of specific steps and/or actions may be modified. Moreover, sub routines or only a portion of a method illustrated in the drawings, such as a small subset of step, may be a separate method. Stated otherwise, some additional methods may include only a portion of the steps shown in a more detailed method.

References to approximations are made throughout this specification, such as by use of the terms "about" or "approximately." For each such reference, it is to be understood that, in some embodiments, the value, feature, or characteristic may be specified without approximation. For example, where qualifiers such as "about," "substantially," and "generally" are used, these terms include within their scope the qualified words in the absence of their qualifiers.

Reference throughout this specification to "an embodiment" or "the embodiment" means that a particular feature, structure or characteristic described in connection with that embodiment is included in at least one embodiment. Thus, the quoted phrases, or variations thereof, as recited throughout this specification are not necessarily all referring to the same embodiment.

Similarly, it should be appreciated that in the above description of embodiments, various features are sometimes grouped together in a single embodiment, figure, or description thereof for the purpose of streamlining the disclosure. This method of disclosure, however, is not to be interpreted as reflecting an intention that any claim require more features than those expressly recited in that claim. Rather, as the following claims reflect, inventive aspects lie in a combination of fewer than all features of any single foregoing disclosed embodiment.

The claims following this written disclosure are hereby expressly incorporated into the present written disclosure,

with each claim standing on its own as a separate embodiment. This disclosure includes all permutations of the independent claims with their dependent claims. Moreover, additional embodiments capable of derivation from the independent and dependent claims that follow are also expressly incorporated into the present written description.

Recitation in the claims of the term “first” with respect to a feature or element does not necessarily imply the existence of a second or additional such feature or element. Elements specifically recited in means-plus-function format, if any, are intended to be construed in accordance with 35 U.S.C. § 112 ¶6. Embodiments of the invention in which an exclusive property or privilege is claimed are defined as follows.

The invention claimed is:

1. A method of treating cardiac complex rhythm disorder in a patient, the method comprising:

positioning a sensor system at a first position within a heart of a patient, wherein the sensor system comprises a sensing region;

receiving a plurality of electrical signals from the sensor system, wherein each electrical signal is detected at a separate sensor location on a cardiac wall of the heart, and wherein each electrical signal comprises an electrogram waveform;

simultaneously receiving an electrical base signal of the heart comprising a base signal frequency and a base signal waveform;

ranking the electrical signals relative to each other based on at least a timing and a frequency of the electrogram waveform of each electrical signal that is distinguishable from the base signal frequency;

determining, based on the ranking of the electrical signals, that a source of aberrant electrical activity is disposed at a location on the cardiac wall that is outside of the sensing region of the sensor system when the sensor system is at the first position, wherein the source generates an electrogram waveform, in at least one of the electrical signals, having a frequency distinguishable from the base signal frequency; and

repositioning the sensor system at a second position within the heart.

2. The method of claim 1, wherein the ranking of the electrical signals provides a direction for moving the sensor system in the repositioning step.

3. The method of claim 1, wherein an electrical signal having an electrogram waveform with a higher frequency receives a higher ranking than an electrical signal having an electrogram waveform with a lower frequency.

4. The method of claim 1, wherein the ranking comprises weighting each electrical signal based on characteristics of its electrogram waveform, wherein higher frequency is weighted heavier than lower frequency.

5. The method of claim 1, further comprising: identifying a target site on the cardiac wall that corresponds to the location of the source of aberrant electrical activity, wherein the target site is within the sensing region of the sensor system at the second position.

6. The method of claim 5, further comprising: treating the target site via ablation.

7. The method of claim 1, further comprising: generating a representative image of the heart of the patient; and

identifying a target position on the representative image that corresponds to the location of the source of aberrant electrical activity.

8. The method of claim 1, wherein ranking the electrical signals relative to each other comprises:

determining whether the electrogram waveform of at least two electrical signals show propagation of a wavefront, wherein an electrical signal having the wavefront present at an earlier time receives a higher ranking than an electrical signal having the wavefront present at a later time.

9. The method of claim 1, wherein ranking the electrical signals relative to each other comprises:

determining that at least some of the electrogram waveforms show propagation of a first wavefront; and assigning a higher ranking to an electrical signal in which the first wavefront is present at an earlier time, as compared with a ranking of an electrical signal in which the first wavefront is present at a later time.

10. The method of claim 9, wherein some of the electrical signals comprise a second wavefront, wherein the first wavefront reoccurs at a first frequency, wherein the second wavefront reoccurs at a second frequency that is lower than the first frequency, and wherein ranking the electrical signals relative to each other comprises assigning electrical signals that comprise the first wavefront a higher ranking than electrical signals that comprise the second wavefront.

11. The method of claim 9, further comprising receiving a plurality of additional electrical signals from the sensor system after the sensor system has been repositioned to the second position, wherein each additional electrical signal corresponds with a separate location on the cardiac wall of the heart of the patient, wherein each additional electrical signal comprises an electrogram waveform, and wherein at least some of the plurality of additional electrical signals comprise a second wavefront reoccurring at a frequency similar to a reoccurrence of the first wavefront; and

ranking the plurality of additional electrical signals relative to each other by assigning a higher ranking to an additional electrical signal in which the second wavefront is present at an earlier time, as compared with a ranking of an additional electrical signal in which the second wavefront is present at a later time.

12. The method of claim 11, further comprising identifying a target site of the cardiac wall based on the ranking of the plurality of additional electrical signals, wherein the target site corresponds with a location on the cardiac wall that corresponds with the additional electrical signal that receives the highest ranking.

13. The method of claim 11, further comprising identifying a target site of the cardiac wall, wherein identifying the target site comprises interpolating a location of the target site from locations on the cardiac wall that correspond with at least some of the additional electrical signals that have been ranked.

14. The method of claim 1, wherein electrical signals transmitting from pulmonary veins are isolated from the cardiac wall via tissue ablation prior to receiving the plurality of electrical signals from the sensor system.

15. A method of treating cardiac complex rhythm disorder in a patient, the method comprising:

positioning a plurality of sensors at a first position within a heart of a patient, wherein the plurality of sensors define a sensing region;

receiving a plurality of electrical signals from the plurality of sensors that are interior to a wall of the heart of, wherein each electrical signal corresponds with a separate location on a cardiac wall of the heart, and wherein each electrical signal comprises an electrogram waveform;

simultaneously receiving an electrical base signal of the heart comprising a base signal frequency and a base signal waveform; and
 ranking the electrical signals relative to each other to identify a location on the cardiac wall of the heart that is a source of aberrant electrical activity; wherein the source generates a waveform with a frequency distinguishable from the base signal frequency in at least one of the electrical signals;
 determining, based on the ranking of the electrical signals, that the location of the source of aberrant electrical activity is outside of the sensing region of the plurality of sensors when the plurality of sensors are at the first position; and
 repositioning the plurality of sensors at a second position within the heart.

16. The method of claim 15, wherein ranking the electrical signals relative to each other is to further identify an additional location on the cardiac wall of the heart that is an additional source of aberrant electrical activity, and wherein the sources of aberrant electrical activity are spaced from each other.

17. The method of claim 15, wherein the ranking is based on at least a frequency of the electrogram waveform of each electrical signal, and wherein an electrical signal having an electrogram waveform with a higher frequency receives a higher ranking than an electrical signal having an electrogram waveform with a lower frequency.

18. The method of claim 15, wherein the ranking is based on at least a frequency of the electrogram waveform of each electrical signal, wherein the ranking comprises weighting each electrical signal based on characteristics of its electrogram waveform, and wherein higher frequency is weighted heavier than lower frequency.

19. The method of claim 15, further comprising:
 identifying a target site on the cardiac wall that corresponds to the location of the source of aberrant electrical activity, wherein the target site is within the sensing region of the plurality of sensors at the second position.

20. The method of claim 19, further comprising:
 treating the target site via ablation.

21. The method of claim 15, further comprising:
 generating a representative image of the heart of the patient; and
 identifying a target position on the representative image that corresponds to the location of the source of aberrant electrical activity.

22. The method of claim 15, wherein ranking the electrical signals relative to each other comprises:
 determining whether the electrogram waveform of at least two electrical signals show propagation of a wavefront, wherein an electrical signal having the wavefront present at an earlier time receives a higher ranking than an electrical signal having the wavefront present at a later time.

23. The method of claim 15, wherein ranking the electrical signals relative to each other comprises:
 determining that at least some of the electrogram waveforms show propagation of a first wavefront; and
 assigning a higher ranking to an electrical signal in which the first wavefront is present at an earlier time, as compared with a ranking of an electrical signal in which the first wavefront is present at a later time.

24. The method of claim 23, wherein some of the electrical signals comprise a second wavefront, wherein the first wavefront reoccurs at a first frequency, wherein the second

wavefront reoccurs at a second frequency that is lower than the first frequency, and wherein ranking the electrical signals relative to each other comprises assigning electrical signals that comprise the first wavefront a higher ranking than electrical signals that comprise the second wavefront.

25. The method of claim 23, further comprising receiving a plurality of additional electrical signals from the plurality of sensors after the plurality of sensors have been repositioned to the second position, wherein each additional electrical signal corresponds with a separate location on the cardiac wall of the heart of the patient, wherein each additional electrical signal comprises an electrogram waveform, and wherein at least some of the plurality of additional electrical signals comprise a second wavefront reoccurring at a frequency similar to a reoccurrence of the first wavefront; and

ranking the plurality of additional electrical signals relative to each other by assigning a higher ranking to an additional electrical signal in which the second wavefront is present at an earlier time, as compared with a ranking of an additional electrical signal in which the second wavefront is present at a later time.

26. The method of claim 25, further comprising identifying a target site of the cardiac wall based on the ranking of the plurality of additional electrical signals, wherein the target site corresponds with a location on the cardiac wall that corresponds with the additional electrical signal that receives the highest ranking.

27. The method of claim 25, further comprising identifying a target site of the cardiac wall, wherein identifying the target site comprises interpolating a location of the target site from locations on the cardiac wall that correspond with at least some of the additional electrical signals that have been ranked.

28. The method of claim 15, wherein electrical signals transmitting from pulmonary veins are isolated from the cardiac wall via tissue ablation prior to receiving the plurality of electrical signals from the plurality of sensors.

29. A computer-implemented method of treating cardiac complex rhythm disorder in a patient, the method comprising:

positioning a sensor system at a first position within a heart of a patient, wherein the sensor system comprises a sensing region;

receiving, on a computing device, a plurality of electrical signals from the sensor system, wherein each electrical signal corresponds with a separate location on a cardiac wall of the heart, and wherein each electrical signal comprises an electrogram waveform;

simultaneously receiving an electrical base signal of the heart comprising a base signal frequency and a base signal waveform;

ranking, via the computing device, the electrical signals relative to each other based on at least one of a timing and a frequency of the electrogram waveform of each electrical signal that is distinguishable from the base signal;

determining, based on the ranking of the electrical signals, that a source of errant electrical activity is disposed at a location on the cardiac wall that is outside of the sensing region of the sensor system when the sensor system is at the first position, wherein the source generates an electrogram waveform, in at least one of the electrical signals, having a frequency distinguishable from the base signal frequency; and

repositioning the sensor system at a second position within the heart.

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30. The method of claim 29, wherein an electrical signal having an electrogram waveform with a higher frequency receives a higher ranking than an electrical signal having an electrogram waveform with a lower frequency.

31. The method of claim 29, wherein the ranking comprises weighting each electrical signal based on characteristics of its electrogram waveform, wherein higher frequency is weighted heavier than lower frequency.

32. The method of claim 29, further comprising:

identifying, via the computing device, a target site on the cardiac wall that corresponds to the location of the source of errant electrical activity, wherein the target site is within the sensing region of the sensor system at the second position.

33. The method of claim 32, further comprising: treating the target site via ablation.

34. The method of claim 29, further comprising:

generating, via the computing device, a representative image of the heart of the patient; and

identifying, via the computing device, a target position on the representative image that corresponds to the location of the source of errant electrical activity.

35. The method of claim 29, wherein ranking the electrical signals relative to each other comprises:

determining whether the electrogram waveform of at least two electrical signals show propagation of a wavefront, wherein an electrical signal having the wavefront present at an earlier time receives a higher ranking than an electrical signal having the wavefront present at a later time.

36. The method of claim 29, wherein ranking the electrical signals relative to each other comprises:

determining that at least some of the electrogram waveforms show propagation of a first wavefront; and assigning a higher ranking to an electrical signal in which the first wavefront is present at an earlier time, as compared with a ranking of an electrical signal in which the first wavefront is present at a later time.

37. The method of claim 36, wherein some of the electrical signals comprise a second wavefront, wherein the first wavefront reoccurs at a first frequency, wherein the second

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wavefront reoccurs at a second frequency that is lower than the first frequency, and wherein ranking the electrical signals relative to each other comprises assigning electrical signals that comprise the first wavefront a higher ranking than electrical signals that comprise the second wavefront.

38. The method of claim 36, further comprising receiving a plurality of additional electrical signals from the sensor system after the sensor system has been repositioned to the second position, wherein each additional electrical signal corresponds with a separate location on the cardiac wall of the heart of the patient, wherein each additional electrical signal comprises an electrogram waveform, and wherein at least some of the plurality of additional electrical signals comprise a second wavefront reoccurring at a frequency similar to a reoccurrence of the first wavefront; and

ranking the plurality of additional electrical signals relative to each other by assigning a higher ranking to an additional electrical signal in which the second wavefront is present at an earlier time, as compared with a ranking of an additional electrical signal in which the second wavefront is present at a later time.

39. The method of claim 38, further comprising identifying a target site of the cardiac wall based on the ranking of the plurality of additional electrical signals, wherein the target site corresponds with a location on the cardiac wall that corresponds with the additional electrical signal that receives the highest ranking.

40. The method of claim 38, further comprising identifying a target site of the cardiac wall, wherein identifying the target site comprises interpolating a location of the target site from locations on the cardiac wall that correspond with at least some of the additional electrical signals that have been ranked.

41. The method of claim 29, wherein electrical signals transmitting from pulmonary veins are isolated from the cardiac wall via tissue ablation prior to receiving the plurality of electrical signals from the sensor system.

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专利名称(译)	心房颤动治疗系统和方法		
公开(公告)号	US10010258	公开(公告)日	2018-07-03
申请号	US15/047670	申请日	2016-02-19
[标]申请(专利权)人(译)	INTERMOUNTAIN技术管理		
申请(专利权)人(译)	INTERMOUNTAIN技术管理有限责任公司		
[标]发明人	BUNCH THOMAS JARED DAY JOHN DAVID		
发明人	BUNCH, THOMAS JARED DAY, JOHN DAVID		
IPC分类号	A61B5/046 A61B5/04 A61B5/00		
CPC分类号	A61B5/046 A61B5/7264 A61B5/6869 A61B5/04012 G16H50/20		
审查员(译)	DIETRICH , JOSEPH		
优先权	61/662323 2012-06-20 US 61/799242 2013-03-15 US 61/798456 2013-03-15 US		
其他公开文献	US20160166166A1		
外部链接	Espacenet		

摘要(译)

用于治疗患者的心脏复杂节律紊乱的方法可包括从传感器系统接收多个电信号，其中每个电信号对应于患者心脏的心壁上的单独位置，并且其中每个电信号包括电描记图波形；并且至少基于每个电信号的电描记图波形的均匀性和频率对电信号相对于彼此进行排序。

