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(54) **METHOD AND APPARATUS FOR ATRIAL ARRHYTHMIA EPISODE DETECTION**

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(71) Applicant: **Medtronic, Inc.**, Minneapolis, MN (US)

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(72) Inventors: **Shantanu Sarkar**, Roseville, MN (US);
Daniel L. Hansen, Castle Rock, CO (US);
Grant A. Neitzell, Fridley, MN (US)

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(73) Assignee: **Medtronic, Inc.**, Minneapolis, MN (US)

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Related U.S. Application Data

(57) **ABSTRACT**

(60) Provisional application No. 62/117,785, filed on Feb. 18, 2015.

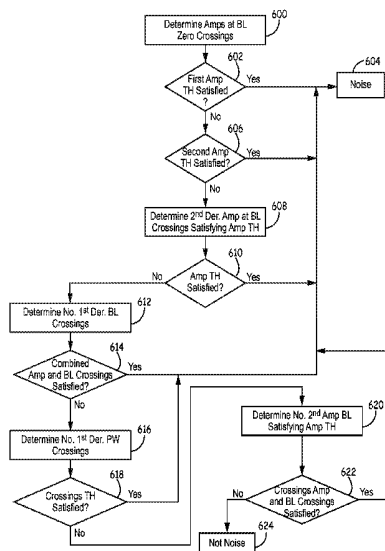
A method and implantable medical device for determining noise in response to a cardiac signal that includes sensing the cardiac signal, determining a sensing window in response to the sensed cardiac signal, the sensing window comprising a first portion and a second portion, determining a first derivative signal in response to the sensed cardiac signal within only one of the first portion and the second portion of the sensing window, determining a second derivative signal in response to the sensed cardiac signal within the one of the first portion and the second portion of the sensing window, determining whether an amplitude of the second derivative signal satisfies an amplitude threshold, and determining noise in response to the amplitude of the second derivative signal satisfying the amplitude threshold.

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A61N 1/3718; **A61N 1/37**
See application file for complete search history.

32 Claims, 7 Drawing Sheets



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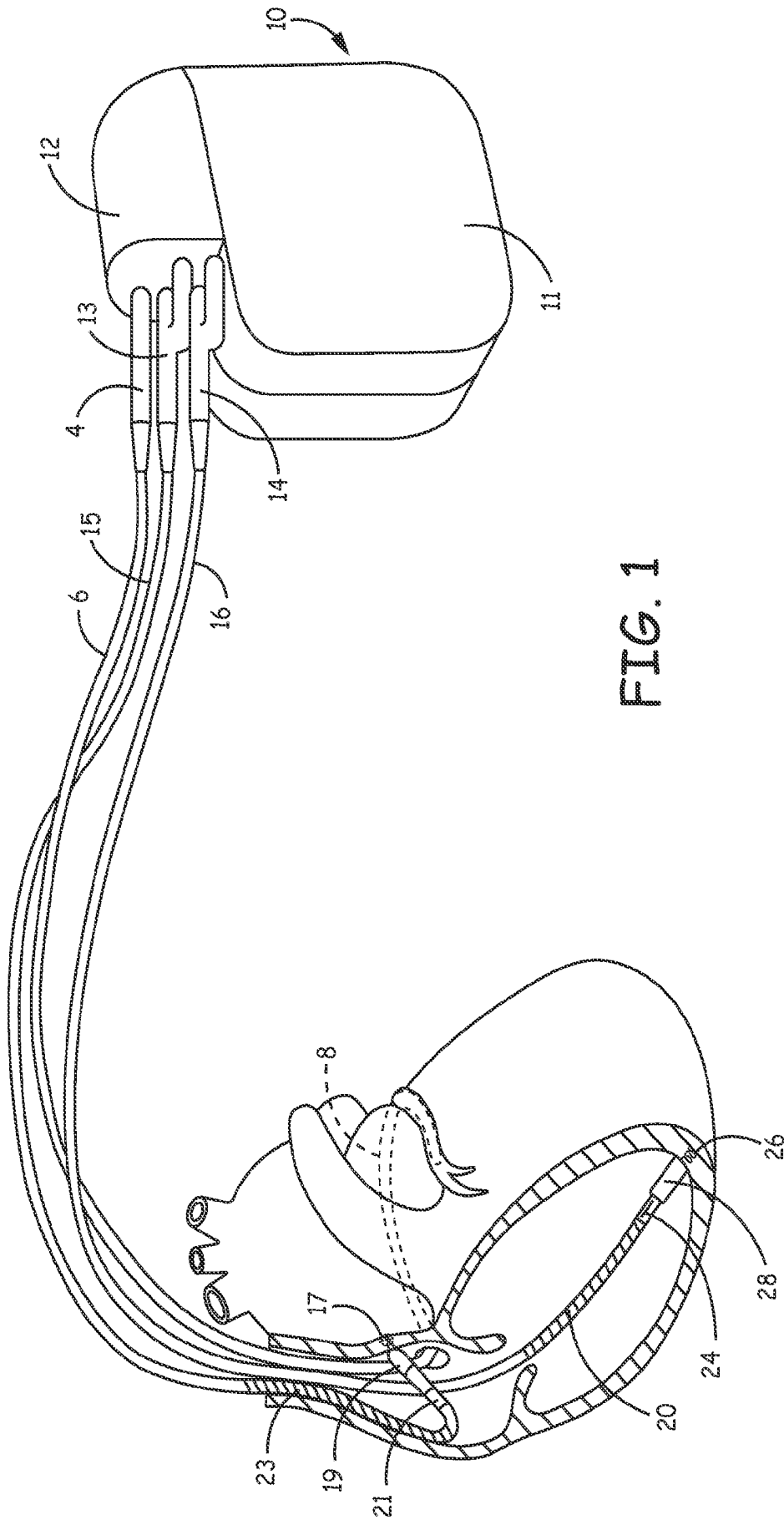


FIG. 1

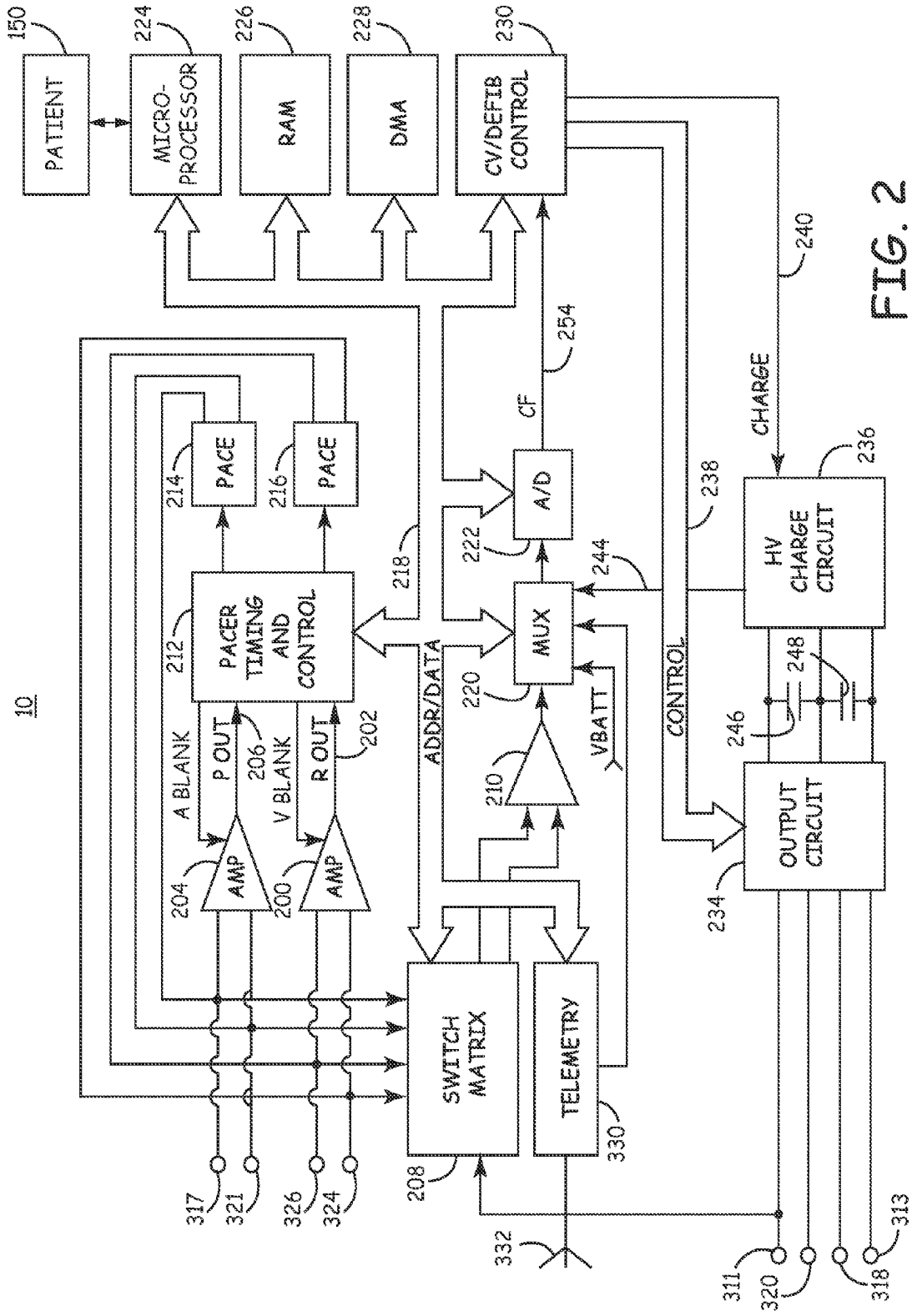


FIG. 2

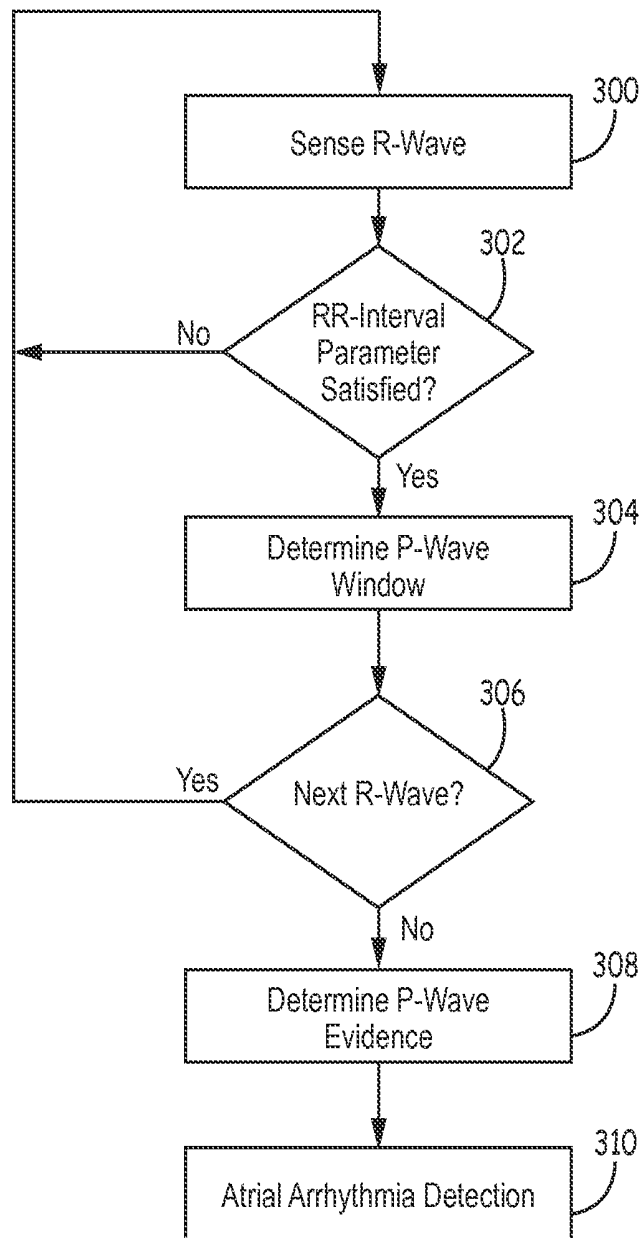


FIG. 3

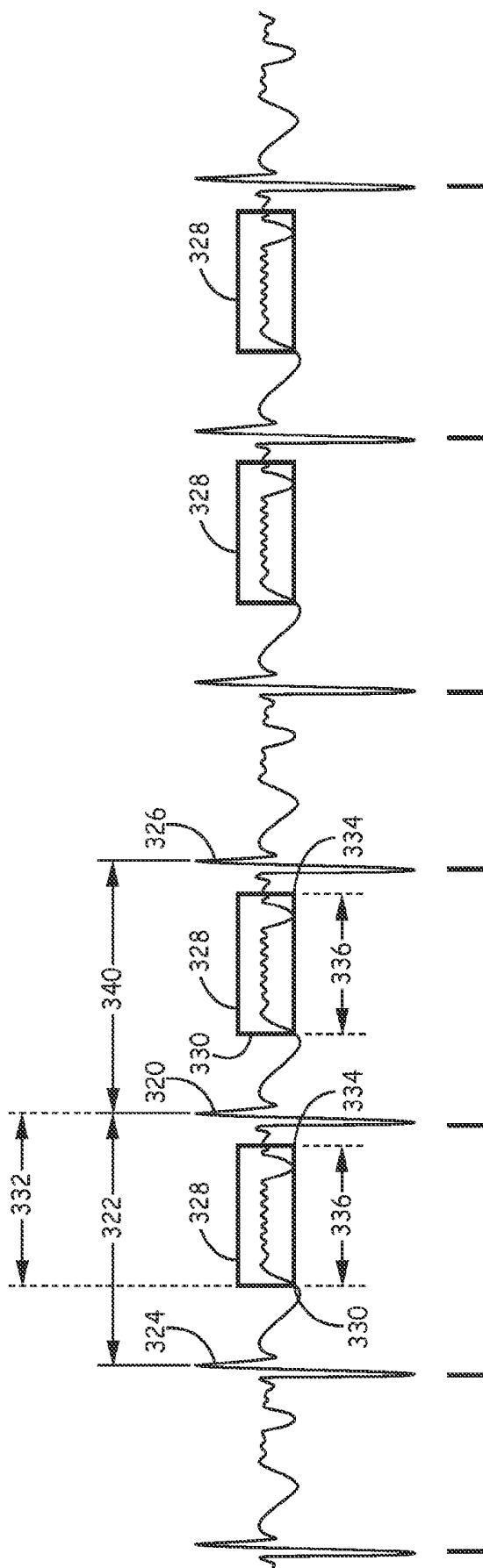


FIG. 4

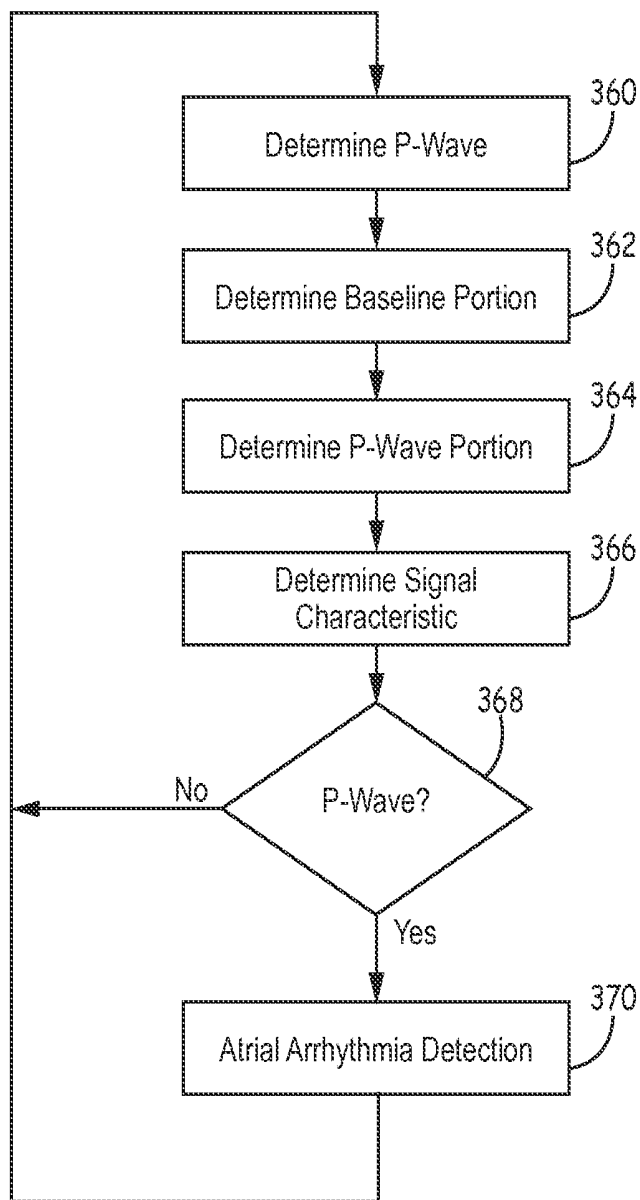


FIG. 5

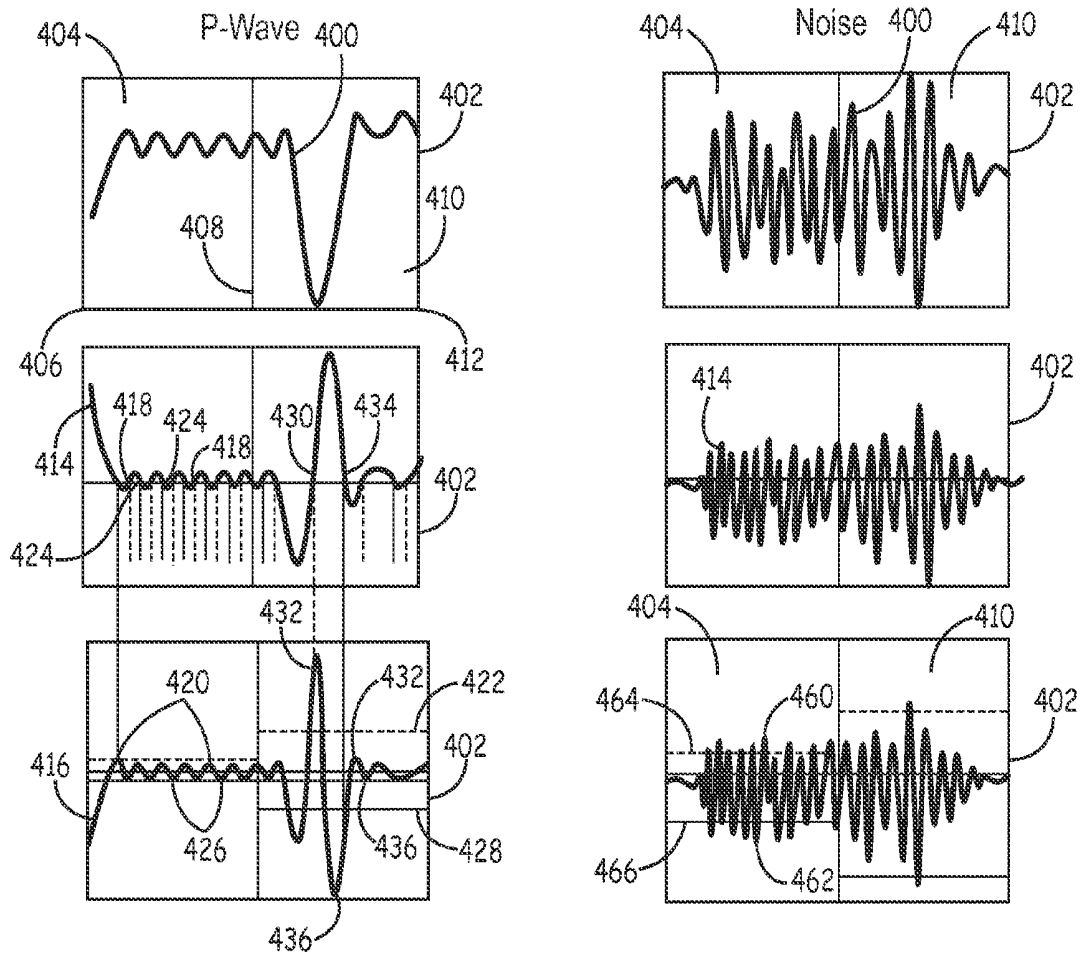


FIG. 6

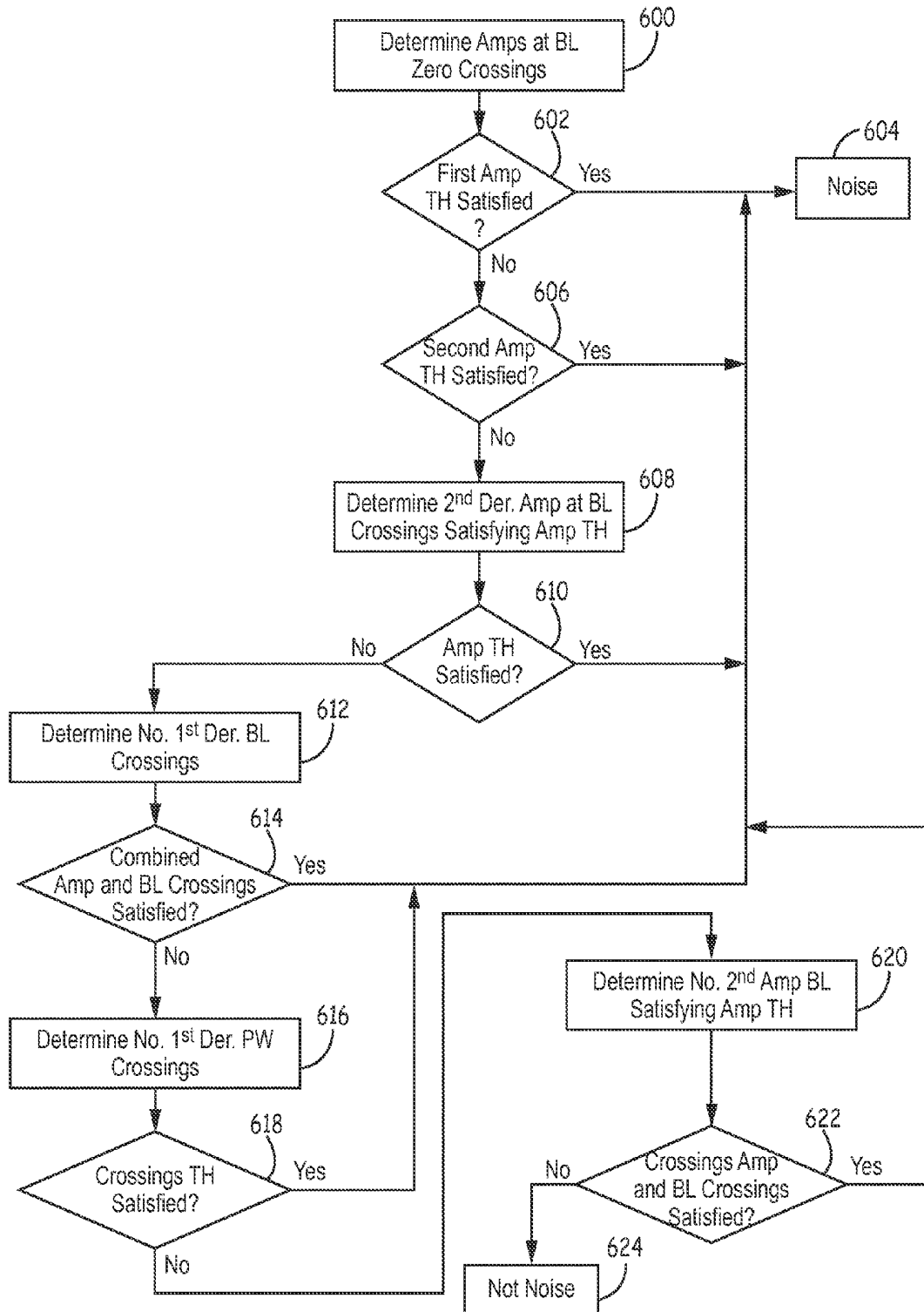


FIG. 7

METHOD AND APPARATUS FOR ATRIAL ARRHYTHMIA EPISODE DETECTION

CROSS-REFERENCE TO RELATED APPLICATIONS

This application claims the benefit of U.S. Provisional Application No. 62/117,785, filed on Feb. 18, 2015, incorporated herein by reference in its entirety.

TECHNICAL FIELD

The disclosure relates generally to implantable cardiac medical devices and, in particular, to a method for and apparatus for detecting atrial tachyarrhythmia episodes in an implantable cardiac medical device.

BACKGROUND

During normal sinus rhythm (NSR), the heart beat is regulated by electrical signals produced by the sino-atrial (SA) node located in the right atrial wall. Each atrial depolarization signal produced by the SA node spreads across the atria, causing the depolarization and contraction of the atria, and arrives at the atrioventricular (A-V) node. The A-V node responds by propagating a ventricular depolarization signal through the bundle of His of the ventricular septum and thereafter to the bundle branches and the Purkinje muscle fibers of the right and left ventricles.

Atrial tachyarrhythmia includes the disorganized form of atrial fibrillation and varying degrees of organized atrial tachycardia, including atrial flutter. Atrial fibrillation (AF) occurs because of multiple focal triggers in the atrium or because of changes in the substrate of the atrium causing heterogeneities in conduction through different regions of the atria. The ectopic triggers can originate anywhere in the left or right atrium or pulmonary veins. The AV node will be bombarded by frequent and irregular atrial activations but will only conduct a depolarization signal when the AV node is not refractory. The ventricular cycle lengths will be irregular and will depend on the different states of refractoriness of the AV-node.

In the past, atrial arrhythmias have been largely under-treated due to the perception that these arrhythmias are relatively benign. As more serious consequences of persistent atrial arrhythmias have come to be understood, such as an associated risk of relatively more serious ventricular arrhythmias and stroke, there is a growing interest in monitoring and treating atrial arrhythmias.

Methods for discriminating arrhythmias that are atrial in origin from arrhythmias originating in the ventricles have been developed for use in dual chamber implantable devices wherein both an atrial EGM signal and a ventricular EGM signal are available. Discrimination of arrhythmias can rely on event intervals (PP intervals and RR intervals), event patterns, and EGM morphology. Such methods have been shown to reliably discriminate ventricular arrhythmias from supra-ventricular arrhythmias. In addition, such methods have been developed for use in single chamber implantable devices, subcutaneous implantable devices, and external monitoring devices, where an adequate atrial EGM signal having acceptable signal-to-noise ratio is not always available for use in detecting and discriminating atrial arrhythmias.

Occasionally, false detection of atrial fibrillation may occur in a subcutaneous device during runs of ectopic rhythm with irregular coupling intervals or underlying sinus

variability/sick sinus. In addition, false detection of atrial tachycardia may occur in a subcutaneous device during ectopy and regular normal sinus rhythm. Therefore, what is needed is a method for improving detection of atrial tachyarrhythmia to reduce false detection in a medical device.

BRIEF DESCRIPTION OF THE DRAWINGS

FIG. 1 is a schematic diagram of an exemplary medical device for detecting an arrhythmia according to an embodiment of the present disclosure.

FIG. 2 is a functional schematic diagram of the medical device of FIG. 1.

FIG. 3 is a flowchart of a method for detecting an atrial arrhythmia according to an embodiment of the disclosure.

FIG. 4 is a schematic diagram of detecting an atrial arrhythmia according to an embodiment of the disclosure.

FIG. 5 is a flowchart of a method of detecting an atrial arrhythmia in a medical device according to an embodiment of the disclosure.

FIG. 6 is a schematic diagram of detecting an atrial arrhythmia in a medical device, according to an embodiment of the disclosure.

FIG. 7 is a flowchart of a method of determining an atrial arrhythmia according to an embodiment of the disclosure.

DETAILED DESCRIPTION

In the following description, references are made to illustrative embodiments for carrying out the methods described herein. It is understood that other embodiments may be utilized without departing from the scope of the disclosure.

In various embodiments, ventricular signals are used for determining successive ventricular cycle lengths for use in detecting atrial arrhythmias. The atrial arrhythmia detection methods do not require an electrode positioned within the atrium as an atrial signal source to directly sense the atrial signal within the heart; i.e., the device may be a single chamber device having an electrode positioned only within the ventricle, or a subcutaneous device having no electrode positioned within the heart. The methods presented herein may be embodied in software, hardware or firmware in implantable or external medical devices. Such devices include implantable monitoring devices having cardiac EGM/ECG monitoring capabilities and associated EGM/ECG sense electrodes, which may be intracardiac, epicardial, or subcutaneous electrodes.

The methods described herein can also be incorporated in implantable medical devices having therapy delivery capabilities, such as single chamber or bi-ventricular pacing systems or ICDs that sense the R-waves in the ventricles and deliver an electrical stimulation therapy to the ventricles. The atrial arrhythmia detection methods presently disclosed may also be incorporated in external monitors having ECG electrodes coupled to the patient's skin to detect R-waves, e.g. Holter monitors, or within computerized systems that analyze pre-recorded ECG or EGM data. Embodiments may further be implemented in a patient monitoring system, such as a centralized computer system which processes data sent to it by implantable or wearable monitoring devices, including subcutaneous devices having loop recorders.

FIG. 1 is a schematic diagram of an exemplary medical device for detecting an arrhythmia according to an embodiment of the present disclosure. As illustrated in FIG. 1, a medical device according to an embodiment of the present disclosure may be in the form of an implantable cardioverter

defibrillator (ICD) **10** a connector block **12** that receives the proximal ends of a right ventricular lead **16**, a right atrial lead **15** and a coronary sinus lead **6**, used for positioning electrodes for sensing and stimulation in three or four heart chambers. Right ventricular lead **16** is positioned such that its distal end is in the right ventricle for sensing right ventricular cardiac signals and delivering pacing or shocking pulses in the right ventricle. For these purposes, right ventricular lead **16** is equipped with a ring electrode **24**, an extendable helix electrode **26** mounted retractably within an electrode head **28**, and a coil electrode **20**, each of which are connected to an insulated conductor within the body of lead **16**. The proximal end of the insulated conductors are coupled to corresponding connectors carried by bifurcated connector **14** at the proximal end of lead **16** for providing electrical connection to the ICD **10**. It is understood that although the device illustrated in FIG. **1** is a dual chamber device, other devices such as single chamber devices may be utilized to perform the technique of the present disclosure described herein.

The right atrial lead **15** is positioned such that its distal end is in the vicinity of the right atrium and the superior vena cava. Lead **15** is equipped with a ring electrode **21** and an extendable helix electrode **17**, mounted retractably within electrode head **19**, for sensing and pacing in the right atrium. Lead **15** is further equipped with a coil electrode **23** for delivering high-energy shock therapy. The ring electrode **21**, the helix electrode **17** and the coil electrode **23** are each connected to an insulated conductor with the body of the right atrial lead **15**. Each insulated conductor is coupled at its proximal end to a connector carried by bifurcated connector **13**.

The coronary sinus lead **6** is advanced within the vasculature of the left side of the heart via the coronary sinus and great cardiac vein. The coronary sinus lead **6** is shown in the embodiment of FIG. **1** as having a defibrillation coil electrode **8** that may be used in combination with either the coil electrode **20** or the coil electrode **23** for delivering electrical shocks for cardioversion and defibrillation therapies. In other embodiments, coronary sinus lead **6** may also be equipped with a distal tip electrode and ring electrode for pacing and sensing functions in the left chambers of the heart. The coil electrode **8** is coupled to an insulated conductor within the body of lead **6**, which provides connection to the proximal connector **4**.

The electrodes **17** and **21** or **24** and **26** may be used as true bipolar pairs, commonly referred to as a "tip-to-ring" configuration. Further, electrode **17** and coil electrode **20** or electrode **24** and coil electrode **23** may be used as integrated bipolar pairs, commonly referred to as a "tip-to-coil" configuration. In accordance with the invention, ICD **10** may, for example, adjust the electrode configuration from a tip-to-ring configuration, e.g., true bipolar sensing, to a tip-to-coil configuration, e.g., integrated bipolar sensing, upon detection of oversensing in order to reduce the likelihood of future oversensing. In other words, the electrode polarities can be reselected in response to detection of oversensing in an effort to reduce susceptibility of oversensing. In some cases, electrodes **17**, **21**, **24**, and **26** may be used individually in a unipolar configuration with the device housing **11** serving as the indifferent electrode, commonly referred to as the "can" or "case" electrode.

The device housing **11** may also serve as a subcutaneous defibrillation electrode in combination with one or more of the defibrillation coil electrodes **8**, **20** or **23** for defibrillation of the atria or ventricles. It is recognized that alternate lead systems may be substituted for the three lead system illus-

trated in FIG. **1**. While a particular multi-chamber ICD and lead system is illustrated in FIG. **1**, methodologies included in the present invention may adapted for use with any single chamber, dual chamber, or multi-chamber ICD or pacemaker system, subcutaneous implantable device, or other internal or external cardiac monitoring device.

ICD **10** may alternatively be configured as a subcutaneous device having sensing or pacing electrodes incorporated on the housing **11** of the device in which case transvenous leads are not required. A subcutaneous device may be coupled to a lead tunneled subcutaneously or submuscularly for delivering transthoracic pacing pulses and/or sensing ECG signals. An exemplary subcutaneous device is described in commonly assigned U.S. patent application Ser. Nos. 14/604,111 and 14/604,260, both incorporated herein by reference in their entireties. The techniques described herein can also be implemented in an external device, e.g. including patch electrodes and optionally another physiological sensor if desired, that can sense variable parameters as described herein.

FIG. **2** is a functional schematic diagram of the medical device of FIG. **1**. This diagram should be taken as exemplary of the type of device with which the invention may be embodied and not as limiting. The disclosed embodiment shown in FIG. **2** is a microprocessor-controlled device, but the methods of the present invention may also be practiced with other types of devices such as those employing dedicated digital circuitry.

With regard to the electrode system illustrated in FIG. **1**, ICD **10** is provided with a number of connection terminals for achieving electrical connection to the leads **6**, **15**, and **16** and their respective electrodes. A connection terminal **311** provides electrical connection to the housing **11** for use as the indifferent electrode during unipolar stimulation or sensing. The connection terminals **320**, **313**, and **318** provide electrical connection to coil electrodes **20**, **8** and **23** respectively. Each of these connection terminals **311**, **320**, **313**, and **318** are coupled to the high voltage output circuit **234** to facilitate the delivery of high energy shocking pulses to the heart using one or more of the coil electrodes **8**, **20**, and **23** and optionally the housing **11**.

The connection terminals **317** and **321** provide electrical connection to the helix electrode **17** and the ring electrode **21** positioned in the right atrium. The connection terminals **317** and **321** are further coupled to an atrial sense amplifier **204** for sensing atrial signals such as P-waves. The connection terminals **326** and **324** provide electrical connection to the helix electrode **26** and the ring electrode **24** positioned in the right ventricle. The connection terminals **326** and **324** are further coupled to a ventricular sense amplifier **200** for sensing ventricular signals. The atrial sense amplifier **204** and the ventricular sense amplifier **200** preferably take the form of automatic gain controlled amplifiers with adjustable sensitivity. In accordance with the invention, ICD **10** and, more specifically, microprocessor **224** automatically adjusts the sensitivity of atrial sense amplifier **204**, ventricular sense amplifier **200** or both in response to detection of oversensing in order to reduce the likelihood of oversensing. Ventricular sense amplifier **200** and atrial sense amplifier **204** operate in accordance with originally programmed sensing parameters for a plurality of cardiac cycles, and upon detecting oversensing, automatically provides the corrective action to avoid future oversensing. In this manner, the adjustments provided by ICD **10** to amplifiers **200** and **204** to avoid future oversensing are dynamic in nature. Particularly, microprocessor **224** increases a sensitivity value of the amplifiers, thus reducing the sensitivity, when oversensing is

detected. Atrial sense amplifier **204** and ventricular sense amplifier **200** receive timing information from pacer timing and control circuitry **212**.

Specifically, atrial sense amplifier **204** and ventricular sense amplifier **200** receive blanking period input, e.g., ABLANK and VBLANK, respectively, which indicates the amount of time the electrodes are “turned off” in order to prevent saturation due to an applied pacing pulse or defibrillation shock. As will be described, the blanking periods of atrial sense amplifier **204** and ventricular sense amplifier **200** and, in turn, the blanking periods of sensing electrodes associated with the respective amplifiers may be automatically adjusted by ICD **10** to reduce the likelihood of oversensing. The general operation of the ventricular sense amplifier **200** and the atrial sense amplifier **204** may correspond to that disclosed in U.S. Pat. No. 5,117,824, by Keimel, et al., incorporated herein by reference in its entirety. Whenever a signal received by atrial sense amplifier **204** exceeds an atrial sensitivity, a signal is generated on the P-out signal line **206**. Whenever a signal received by the ventricular sense amplifier **200** exceeds a ventricular sensitivity, a signal is generated on the R-out signal line **202**.

Switch matrix **208** is used to select which of the available electrodes are coupled to a wide band amplifier **210** for use in digital signal analysis. Selection of the electrodes is controlled by the microprocessor **224** via data/address bus **218**. The selected electrode configuration may be varied as desired for the various sensing, pacing, cardioversion and defibrillation functions of the ICD **10**. Specifically, microprocessor **224** may modify the electrode configurations based on detection of oversensing due to cardiac or non-cardiac origins. Upon detection of R-wave oversensing, for example, microprocessor **224** may modify the electrode configuration of the right ventricle from true bipolar sensing, e.g., tip-to-ring, to integrated bipolar sensing, e.g., tip-to-coil.

Signals from the electrodes selected for coupling to bandpass amplifier **210** are provided to multiplexer **220**, and thereafter converted to multi-bit digital signals by A/D converter **222**, for storage in random access memory **226** under control of direct memory access circuit **228** via data/address bus **218**. Microprocessor **224** may employ digital signal analysis techniques to characterize the digitized signals stored in random access memory **226** to recognize and classify the patient’s heart rhythm employing any of the numerous signal processing methodologies known in the art. An exemplary tachyarrhythmia recognition system is described in U.S. Pat. No. 5,545,186 issued to Olson et al, incorporated herein by reference in its entirety.

Upon detection of an arrhythmia, an episode of EGM data, along with sensed intervals and corresponding annotations of sensed events, are preferably stored in random access memory **226**. The EGM signals stored may be sensed from programmed near-field and/or far-field sensing electrode pairs. Typically, a near-field sensing electrode pair includes a tip electrode and a ring electrode located in the atrium or the ventricle, such as electrodes **17** and **21** or electrodes **26** and **24**. A far-field sensing electrode pair includes electrodes spaced further apart such as any of: the defibrillation coil electrodes **8**, **20** or **23** with housing **11**; a tip electrode **17** or **26** with housing **11**; a tip electrode **17** or **26** with a defibrillation coil electrode **20** or **23**; or atrial tip electrode **17** with ventricular ring electrode **24**. The use of near-field and far-field EGM sensing of arrhythmia episodes is described in U.S. Pat. No. 5,193,535, issued to Bardy, incorporated herein by reference in its entirety. Annotation of sensed events, which may be displayed and stored with

EGM data, is described in U.S. Pat. No. 4,374,382 issued to Markowitz, incorporated herein by reference in its entirety.

The telemetry circuit **330** receives downlink telemetry from and sends uplink telemetry to an external programmer, as is conventional in implantable anti-arrhythmia devices, by means of an antenna **332**. Data to be uplinked to the programmer and control signals for the telemetry circuit are provided by microprocessor **224** via address/data bus **218**. EGM data that has been stored upon arrhythmia detection or as triggered by other monitoring algorithms may be uplinked to an external programmer using telemetry circuit **330**. Received telemetry is provided to microprocessor **224** via multiplexer **220**. Numerous types of telemetry systems known in the art for use in implantable devices may be used.

The remainder of the circuitry illustrated in FIG. 2 is an exemplary embodiment of circuitry dedicated to providing cardiac pacing, cardioversion and defibrillation therapies. The pacer timing and control circuitry **212** includes programmable digital counters which control the basic time intervals associated with various single, dual or multi-chamber pacing modes or anti-tachycardia pacing therapies delivered in the atria or ventricles. Pacer circuitry **212** also determines the amplitude of the cardiac pacing pulses under the control of microprocessor **224**.

During pacing, escape interval counters within pacer timing and control circuitry **212** are reset upon sensing of R-waves or P-waves as indicated by signals on lines **202** and **206**, respectively. In accordance with the selected mode of pacing, pacing pulses are generated by atrial pacer output circuit **214** and ventricular pacer output circuit **216**. The pacer output circuits **214** and **216** are coupled to the desired electrodes for pacing via switch matrix **208**. The escape interval counters are reset upon generation of pacing pulses, and thereby control the basic timing of cardiac pacing functions, including anti-tachycardia pacing.

The durations of the escape intervals are determined by microprocessor **224** via data/address bus **218**. The value of the count present in the escape interval counters when reset by sensed R-waves or P-waves can be used to measure R-R intervals and P-P intervals for detecting the occurrence of a variety of arrhythmias.

The microprocessor **224** includes associated read-only memory (ROM) in which stored programs controlling the operation of the microprocessor **224** reside. A portion of the random access memory (RAM) **226** may be configured as a number of recirculating buffers capable of holding a series of measured intervals for analysis by the microprocessor **224** for predicting or diagnosing an arrhythmia. In response to the detection of tachycardia, anti-tachycardia pacing therapy can be delivered by loading a regimen from microprocessor **224** into the pacer timing and control circuitry **212** according to the type of tachycardia detected. In the event that higher voltage cardioversion or defibrillation pulses are required, microprocessor **224** activates the cardioversion and defibrillation control circuitry **230** to initiate charging of the high voltage capacitors **246** and **248** via charging circuit **236** under the control of high voltage charging control line **240**. The voltage on the high voltage capacitors is monitored via a voltage capacitor (VCAP) line **244**, which is passed through the multiplexer **220**. When the voltage reaches a predetermined value set by microprocessor **224**, a logic signal is generated on the capacitor full (CF) line **254**, terminating charging. The defibrillation or cardioversion pulse is delivered to the heart under the control of the pacer timing and control circuitry **212** by an output circuit **234** via a control bus **238**. The output circuit **234** determines the

electrodes used for delivering the cardioversion or defibrillation pulse and the pulse wave shape.

In one embodiment, the ICD 10 may be equipped with a patient notification system 150. Any patient notification method known in the art may be used such as generating perceivable twitch stimulation or an audible sound. A patient notification system may include an audio transducer that emits audible sounds including voiced statements or musical tones stored in analog memory and correlated to a programming or interrogation operating algorithm or to a warning trigger event as generally described in U.S. Pat. No. 6,067,473 issued to Greeninger et al., incorporated herein by reference in its entirety.

FIG. 3 is a flowchart of a method for detecting an atrial arrhythmia according to an embodiment of the disclosure. As illustrated in FIG. 3, in order to determine whether a sensed cardiac signal is an atrial tachycardia event, the device determines whether the cardiac signal contains a P-wave portion, the results of which are utilized to augment an atrial tachycardia determination process. For example, the determination as to whether a P-wave is detected may be utilized to augment detection of atrial arrhythmias based on the irregularity of ventricular cycles having RR intervals that exhibit discriminatory signatures when plotted in a Lorenz scatter plot, such as is generally disclosed by Ritscher et al. in U.S. Pat. No. 7,031,765, or in U.S. Pat. No. 8,639,316 to Sarkar, both incorporated herein by reference in their entireties. Other atrial arrhythmia determination methods are generally disclosed by Sarkar, et al. in U.S. Pat. No. 7,623,911 and in U.S. Pat. No. 7,537,569, and by Houben in U.S. Pat. No. 7,627,368, all of which patents are also incorporated herein by reference in their entireties.

According to one embodiment, for example, during determination of signal characteristics for augmenting atrial tachycardia detection, the device senses the cardiac signal and identifies R-waves in response to the sensed cardiac signal using any known cardiac signal sensing and detection scheme, such as that disclosed in U.S. Pat. No. 5,117,824, by Keimel, et al., for example, described above and incorporated herein by reference in its entirety. Upon detection of an R-wave associated with the sensed cardiac signal, Block 300, the device determines whether the R-wave satisfies one or more RR-interval parameters, Block 302, described below. If the RR-interval parameter or parameters are not satisfied, No in Block 302, the device waits for the next sensed R-wave, Block 300 and the process Block 300-302 is repeated using the next R-wave. If the RR-interval parameter or parameters are satisfied, Yes in Block 302, the device determines a P-wave window associated with the R-wave, Block 304, as described below.

Upon determination of the P-wave window, the device determines whether a predetermined number of R-waves have been identified, Block 306. The predetermined number of R-waves required to satisfy the determination in Block 306 may be set as one or more R-waves, and according to one embodiment is set as four R-waves for example. If the predetermined number of R-waves have not been identified and therefore a next R-wave is needed, Yes in Block 306, the device waits for the next sensed R-wave, Block 300 and the process Block 300-306 is repeated using the next R-wave. If the predetermined number of R-waves have been identified and therefore a next R-wave is not needed, No in Block 306, the device determines P-wave evidence, Block 308, described below, and utilizes the determined P-wave evidence to augment atrial arrhythmia detection, Block 310, as

described, for example, in commonly assigned U.S. patent application Ser. No. 14/695,111, incorporated herein by reference in its entirety.

FIG. 4 is a schematic diagram of detecting an atrial arrhythmia according to an embodiment of the disclosure. As illustrated in FIGS. 3 and 4, in order to determine whether a sensed R-wave 320 satisfies the RR-interval parameters in Block 302, the device determines whether an RR interval 322 extending between the current R-wave 320 and a previous sensed R-wave 324 is greater than an interval threshold, such as 780 ms for example. If the RR interval 322 is not greater than the interval threshold, the RR-interval parameter is not satisfied, No in Block 302, and the process is repeated with the next RR interval 326. If the RR interval 322 is greater than the interval threshold, the RR interval parameter is satisfied, Yes in Block 302.

According to another embodiment, additional RR interval parameters may also be included in the determination as to whether the RR interval parameters have been satisfied in Block 302. For example, using R wave 326 as an example, in addition to the determination of whether the associated RR interval 340 satisfies the RR interval threshold, the device may also compare the RR interval 340 associated with the current R wave 326 with one or more previously determined RR intervals, such as interval 322 for example, and determine whether a relative change associated with the current RR-interval 340 is greater than a change threshold, such as 100 ms, for example. If the relative change associated with the current RR-interval is not greater than the change threshold, the RR interval parameter is not satisfied in Block 302. If the relative change associated with the current RR interval is greater than the change threshold, the RR-interval parameter is satisfied in Block 302.

In this way, if one of the RR intervals parameters are not satisfied, no P-wave window determination is made, and the process is repeated with the next R wave. If the RR interval parameter or one of the RR interval parameters are satisfied, the RR interval parameter is satisfied in Block 302, and the device determines a P wave window 328 associated with the R-wave 320 for determining whether the R wave 320 includes an associated P-wave. For example, in order to determine the P wave window 328, the device determines a P-wave window start point 330 located a predetermined distance 332 prior to the R-wave, such as 620 ms for example, and a P wave window endpoint 334 is located at a predetermined distance 336 subsequent to the P wave start point 330, such as 600 ms, for example, so that the P wave window 328 extends 600 ms between the P wave start point 330 and the P wave endpoint 334. Each time a P wave window 328 is determined, a P wave counter is updated by one, until the predetermined number of P wave windows are identified, such as four P wave windows, for example.

FIG. 5 is a flowchart of a method of detecting an atrial arrhythmia in a medical device according to an embodiment of the disclosure. In response to the predetermined number of P-waves being identified, No in Block 306 of FIG. 3, the device determines P-wave evidence for determining whether a P-wave is likely detected, Block 308, and utilizes the determined P-wave evidence to augment atrial arrhythmia detection, Block 310, described, for example, in commonly assigned U.S. patent application Ser. No. 14/695,111, incorporated herein by reference in its entirety. As illustrated in FIG. 5, during the determination of P-wave evidence, the device determines a characteristic P-wave in response to the current determined P-waves, Block 360. For example, according to one embodiment, the device determines an average P-wave from the four determined P-waves that is

identified as the characteristic P-wave. The associated P-wave window is then divided into a baseline portion, Block 362, and a P-wave portion, Block 364, and determines signal characteristics, Block 366, for one or both of the baseline window and the P-wave window. A determination is then made, based on the determined signal characteristics, whether the characteristic P-wave is confirmed as being a P-wave, Block 368.

If the characteristic P-wave is not confirmed as being a P-wave, No in Block 368, the device waits for the next predetermined number of P-waves to be identified, Yes in Block 306 of FIG. 3, and the process, Blocks 360-368, is repeated using the next identified P-waves. If the characteristic P-wave is confirmed as being a P-wave, Yes in Block 368, the device utilizes the determination of a P-wave being present to augment atrial arrhythmia detection, Block 370, as described for example, in commonly assigned U.S. patent application Ser. No. 14/695,111, incorporated herein by reference in its entirety.

FIG. 6 is a schematic diagram of detecting an atrial arrhythmia in a medical device, according to an embodiment of the disclosure. As illustrated in FIGS. 5 and 6, in order to determine P-wave evidence (Block 308 of FIG. 3), the device determines a characteristic P-wave 400 having a characteristic P wave window 402 determined by averaging the determined four P-wave windows, as described above. The device divides the P-wave window 402 into a baseline portion 404, extending from the P-wave window start point 406 to a midpoint of the window 408, and a P-wave portion 410, extending from the midpoint of the window 408 to a P-wave window endpoint 412. The device determines a first derivative of the P-wave signal 414 and a second derivative of the p-wave signal 416, and determines corresponding second derivative values 420 associated with positive going zero crossings 418 of the first derivative signal 414 within the baseline portion 404 of the first derivative signal window 402. In one embodiment, the first derivative of the P wave signal can be computed as the difference between points separated by eight samples, and the second derivative can be computed as the difference between points separated by four sample in the first derivative.

The device determines the maximum amplitude of the second derivative values 420 associated with the positive going zero crossings 418, and the determined maximum amplitude value is then used to generate a first threshold 422 for evaluating the second derivative P-wave signal 416 within the P-wave portion 410 of the second derivative window 402. According to one embodiment, the threshold 422 is set as a multiple of the maximum of the second derivative values 420, such as twice the maximum of the second derivative values 420, for example.

In the same way, the device determines a corresponding second derivative value 426 for each negative going zero crossing 424 of the derivative signal 414 within the baseline portion 404 of the window 402. A minimum amplitude of the second derivative values 426 associated with the negative going first derivative zero crossings 424 is determined, and the determined minimum amplitude value is used to generate a second threshold 428 for evaluating the second derivative P-wave signal 416 within the P-wave portion 410 of the window 402. According to one embodiment, the threshold 428 is set as a multiple of the minimum of the second derivative values 426, such as twice the minimum of the second derivative values 426, for example.

Using the first threshold 422 determined in response to the determined maximum of the second derivative values 420, the device determines, for each positive going zero crossing

430 of the first derivative signal within the P-wave portion 410 of the first derivative window, a corresponding amplitude 432 of the second derivative signal within the P-wave portion 410 of the corresponding second derivative signal 416. The device compares the resulting maximum amplitudes 432 of the second derivative signal 416 signal within the P-wave portion 410 of the window 402 to the first threshold 422. Similarly, using the second threshold 422 determined in response to the determined minimum of the second derivative values 420, the device compares, for one or more negative going zero crossing 434 of the first derivative signal 414, the corresponding minimum amplitude 436 of the second derivative signal 416 signal within the P-wave portion 410 of the window 402 to the second threshold 428.

A P-wave is determined to have occurred, Yes in Block 368 of FIG. 5, if either the number of maximum amplitudes 432 determined to be greater than or equal to the first threshold 422 is equal to one, or the number of minimum amplitudes 432 determined to be less than or equal to the second threshold 428 is equal to one. If both the number of maximum amplitudes 432 determined to be greater than or equal to the first threshold 422 and the number of minimum amplitudes 432 determined to be less than or equal to the second threshold 428 is not equal to one, a P-wave is not determined to have occurred, No in Block 368 of FIG. 5. The result of the determination of whether a P-wave is identified is then used during the determination of an atrial arrhythmia event, as described for example, in commonly assigned U.S. patent application Ser. No. 14/695,111, incorporated herein by reference in its entirety.

FIG. 7 is a flowchart of a method of determining an atrial arrhythmia according to an embodiment of the disclosure. As illustrated in FIGS. 6 and 7, during detection of P-wave evidence, the device may also determine that the event is associated with other events, such as noise, for example. During determination of signal characteristics (Block 366 of FIG. 5), the device may also determine a noise event is occurring in response to any one of a predetermined conditions being met. For example, in order to determine whether a noise event is occurring, the device may determine the amplitudes of the second derivative signal located at both the positive going zero crossing and the negative going zero crossings of the first derivative signal 414 within the baseline portion 404 of the window 402, Block 600, and determine whether both a maximum amplitude 460 of the second derivative signal 416 at a positive zero crossing of the first derivative signal 414 within the baseline portion 404 of the window 402 and a minimum amplitude 462 of the second derivative signal 416 at a negative zero crossing of the first derivative signal 414 within the baseline portion 404 of the window 402 satisfy a first amplitude threshold, Block 602, such as the maximum amplitude being greater than 16 microvolts and the minimum amplitude being less than -16 microvolts, for example.

If the first amplitude threshold is satisfied, Yes in Block 602, noise is identified for the characteristic P-wave 400, Block 604. If the first amplitude threshold is not satisfied, No in Block 602, the device may determine other conditions for indicating noise, such as determining whether either a maximum amplitude 460 of the second derivative signal 416 at a positive zero crossing of the first derivative signal 414 within the baseline portion 404 of the window 402 or a minimum amplitude 462 of the second derivative signal 416 at a negative zero crossing of the first derivative signal 414 within the baseline portion 404 of the window 402 satisfy a second amplitude threshold, Block 606, such as the maxi-

imum amplitude being greater than 49 microvolts or the minimum amplitude being less than -49 microvolts, for example.

If the second amplitude threshold is satisfied, Yes in Block 606, noise is identified for the characteristic P-wave 400, Block 604. If the second amplitude threshold is not satisfied, No in Block 606, the device may determine the number of positive going zero crossings of the first derivative signal 414 within the baseline portion 404 of the window 402 whose corresponding amplitude 460 of the second derivative signal 416 is greater than a maximum amplitude threshold 464, such as 16 microvolts, for example, and the number of negative going zero crossings of the first derivative signal 414 within the baseline portion 404 of the window 402 whose corresponding minimum amplitude 462 of the second derivative signal 416 is less than a minimum amplitude threshold 466, such as -16 microvolts for example, Block 608. A determination is then made as to whether an amplitude threshold is satisfied, Block 610, and if the amplitude threshold is satisfied, Yes in Block 610, noise is identified, Block 604. For example, according to one embodiment, the device determines whether the amplitude threshold is satisfied in Block 610 by determining whether a sum of both the number of positive going zero crossings of the first derivative signal 414 within the baseline portion 404 of the window 402 whose corresponding amplitude 460 of the second derivative signal 416 is greater than the maximum amplitude threshold 464 and the number of negative going zero crossings of the first derivative signal 414 within the baseline portion 404 of the window 402 whose corresponding minimum amplitude 462 of the second derivative signal 416 is less than the minimum amplitude threshold 466 being equal to a predetermined number, such as 3 for example.

If the amplitude threshold is not satisfied, No in Block 610, the device may determine the number of positive zero crossings within the baseline portion 404 of the window 402 and the number of negative zero crossings within the baseline portion 404 of the window 402, Block 612. A determination is made as to whether a combined amplitude threshold and a baseline crossing threshold is satisfied, Block 614, by determining, for example, whether both the sum of the number of positive going zero crossings of the first derivative signal 414 within the baseline portion 404 of the window 402 whose corresponding amplitude 460 of the second derivative signal 416 is greater than the maximum amplitude threshold 464 and the number of negative going zero crossings of the first derivative signal 414 within the baseline portion 404 of the window 402 whose corresponding minimum amplitude 462 of the second derivative signal 416 is less than the minimum amplitude threshold 464 is equal to a predetermined number, such as three for example, and the sum of the number of positive zero crossings within the baseline portion 404 of the window 402 and the number of negative zero crossings within the baseline portion 404 of the window 402 is within a predetermined range, such as greater than four and less than ten, for example.

If the combined amplitude threshold and baseline crossing threshold is satisfied, Yes in Block 614, a noise event is identified, Block 604. If the combined amplitude threshold and a baseline crossing threshold is satisfied, No in Block 614, the device may determine the number of positive going zero crossings and the number of negative going zero crossings of the first derivative signal 414 within the P-wave portion 410 of the window 302, Block 616, and determine whether a zero crossings threshold has been satisfied, Block 618, by determining whether a sum of the determined number of positive going zero crossings and the number of

negative going zero crossings of the first derivative signal 414 is greater than four, for example.

If the zero crossings threshold has been satisfied, Yes in Block 618, a noise event is determined, Block 604. If the zero crossings threshold has not been satisfied, No in Block 618, the device may determine the number of amplitudes 460 of the second derivative signal 416 within the baseline portion 404 of the window 402 that are greater than the maximum threshold 464, and the number of amplitudes 462 of the second derivative signal 416 within the baseline portion 404 of the window 402 that are less than the minimum threshold 466, Block 620.

A determination is made as to whether a combined amplitude and baseline crossings threshold has been satisfied, Block 622, by determining both whether a sum of the number of positive zero crossings within the baseline portion 404 of the window 402 and the number of negative zero crossings within the baseline portion 404 of the window 402 is greater than a baseline crossing threshold, such as four for example, and whether a sum of the number of amplitudes 460 of the second derivative signal 416 within the baseline portion 404 of the window 402 that are greater than the maximum threshold 464, and the number of amplitudes 462 of the second derivative signal 416 within the baseline portion 404 of the window 402 that are less than the minimum threshold 466 is greater than an amplitude threshold, such as 10 samples or 16 microvolts for example.

If the combined amplitude and baseline crossings threshold has been satisfied, Yes in Block 622, a noise event is determined, Block 604. If the combined amplitude and baseline crossings threshold has not been satisfied, No in Block 622, and therefore none of the predetermined conditions, Blocks 602, 606 610, 614, 618 and 622 are met, a noise event is not identified for the current characteristic P-wave 400, Block 624.

It is understood that any single one or combination and order of the predetermined conditions, Blocks 602, 606 610, 614, 618 and 622, may be utilized in determining whether a noise event is identified, and therefore numerous combinations of the conditions, or single ones of the conditions may be utilized in determining a noise event, and therefore the disclosure is not limited to the combination and order of the conditions as illustrated in FIG. 8. In this way, a noise event may be determined in response to one of any of the conditions of Blocks 602, 606 610, 614, 618 and 622.

Therefore, the characteristic signal 400 may be determined to be a noise event if any one of the following noise conditions are met:

N1. $bwinZC_{max} > 156 \text{ ms}$ AND $bwinZC_{min} < -156 \text{ ms}$ (Block 602)

N2. $bwinZC_{max} > 468 \text{ ms}$ OR $bwinZC_{min} < -468 \text{ ms}$ (Block 606)

N3. $bwinZC_pThr + bwinZC_nThr > 3$ (Block 610)

N4. $bwinZC_pThr + bwinZC_nThr = 3$ AND $\{4 < (bwinZC_p + bwinZC_n) < 10\}$ (Block 614)

N5. $pwinZC_p + pwinZC_n > 4$ (Block 618)

N6. $bwinZC_p + bwinZC_n > 4$ AND $bwinPThr + bwinNThr > 10$ (Block 622)

where $bwinZC_{max}$ is the maximum amplitude 460 of the second derivative signal 416 at a positive zero crossing of the first derivative signal 414 within the baseline portion 404 of the window 402, $bwinZC_{min}$ is the minimum amplitude 462 of the second derivative signal 416 at a negative zero crossing of the first derivative signal 414 within the baseline portion 404 of the window 402, and the remaining conditions are as described above.

Thus, an apparatus and method have been presented in the foregoing description with reference to specific embodiments. It is appreciated that various modifications to the referenced embodiments may be made without departing from the scope of the invention as set forth in the following claims.

The invention claimed is:

1. A method of determining noise in response to a cardiac signal in an implantable medical device, comprising:
 - sensing the cardiac signal;
 - determining a sensing window in response to the sensed cardiac signal, the sensing window comprising a first portion and a second portion;
 - determining a first derivative signal in response to the sensed cardiac signal within only one of the first portion and the second portion of the sensing window;
 - determining a second derivative signal in response to the sensed cardiac signal within the one of the first portion and the second portion of the sensing window;
 - determining whether an amplitude of the second derivative signal satisfies an amplitude threshold; and
 - determining noise in response to the amplitude of the second derivative signal satisfying the amplitude threshold.
2. The method of claim 1, wherein the first derivative signal and the second derivative signal are determined within the first portion of the sensing window, further comprising:
 - determining positive and negative zero crossings of the first derivative signal within the first portion;
 - determining whether a maximum amplitude of the second derivative signal at the positive zero crossings and a minimum amplitude of the second derivative signal at the negative zero crossings satisfy the amplitude threshold; and
 - determining noise in response to both the maximum amplitude and the minimum amplitude satisfying the amplitude threshold.
3. The method of claim 1, wherein the first derivative signal and the second derivative signal are determined within the first portion of the sensing window, further comprising:
 - determining positive and negative zero crossings of the first derivative signal within the first portion;
 - determining whether a maximum amplitude of the second derivative signal at the positive zero crossings and a minimum amplitude of the second derivative signal at the negative zero crossings satisfy the amplitude threshold; and
 - determining noise in response to only one of the maximum amplitude and the minimum amplitude satisfying the amplitude threshold.
4. The method of claim 1, wherein the first derivative signal and the second derivative signal are determined within the first portion of the sensing window, further comprising:
 - determining positive and negative zero crossings of the first derivative signal within the first portion;
 - determining a first number of amplitudes of the second derivative signal at the positive going zero crossing that are greater than a first amplitude threshold;
 - determining a second number of amplitudes of the second derivative signal at the negative going zero crossing that are less than a second amplitude threshold;
 - determining a sum of the first number of amplitudes and the second number of amplitudes; and
 - determining noise in response to the determined sum.

5. The method of claim 4, further comprising:
 - determining whether a total number of the positive zero crossings and the negative zero crossings is within a zero crossings sum threshold; and
 - determining noise in response to both the determined sum being greater than an amplitude sum threshold and the total number of the determined positive zero crossings and the negative zero crossings being within the zero crossings sum threshold.
6. The method of claim 1, wherein the first derivative signal and the second derivative signal are determined within the second portion of the sensing window, further comprising:
 - determining positive and negative zero crossings of the first derivative signal within the second portion;
 - determining whether a total number of the determined positive zero crossings and the negative zero crossing is greater than a total zero crossings threshold; and
 - determining noise in response to the total number of the determined positive zero crossings and the negative zero crossing being greater than the total zero crossings threshold.
7. The method of claim 1, wherein the first derivative signal and the second derivative signal are determined within the first portion of the sensing window, further comprising:
 - determining positive and negative zero crossings of the first derivative signal within the first portion;
 - determining whether a total number of the determined positive zero crossings and the negative zero crossings is greater than a total zero crossings threshold;
 - determining a first number of amplitudes of the second derivative signal at the positive going zero crossings of the first derivative signal that are greater than a positive going amplitude threshold;
 - determining a second number of amplitudes of the second derivative signal at the negative going zero crossings of the first derivative signal that are less than a negative going amplitude threshold;
 - determining whether a sum of the first number of amplitudes and the second number of amplitudes is greater than a total amplitude threshold; and
 - determining noise in response to both the total number of the determined positive zero crossings and the negative zero crossings being greater than the total zero crossings threshold and the sum of the first number of amplitudes and the second number of amplitudes being greater than the total amplitude threshold.
8. The method of claim 1, comprising:
 - determining a first noise condition comprising determining whether a maximum amplitude of the second derivative signal at positive zero crossings of the first derivative signal and a minimum amplitude of the second derivative signal at negative zero crossings of the first derivative signal satisfy a first amplitude threshold;
 - determining a second noise condition comprising:
 - determining a first number of amplitudes of the second derivative signal at positive going zero crossings that are greater than a second amplitude threshold; and
 - determining a second number of amplitudes of the second derivative signal at negative going zero crossings that are less than a third amplitude threshold;
 - determining a third noise condition comprising determining a total number of positive zero crossings and

negative zero crossings of the first derivative signal within the first portion of the sensing window;

determining a fourth noise condition comprising determining a total number of positive zero crossings and negative zero crossings of the first derivative signal within the second portion of the sensing window; and determining a fifth noise condition comprising:

determining a total number of positive zero crossings and negative zero crossings greater than a total zero crossings threshold;

determining a first number of amplitudes of the second derivative signal at the positive going zero crossings of the first derivative signal that are greater than a positive going amplitude threshold; and

determining a second number of amplitudes of the second derivative signal at negative going zero crossings of the first derivative signal that are less than a negative going amplitude threshold, wherein noise is determined in response to one of the first noise condition, the second noise condition, the third noise condition, the fourth noise condition and the fifth noise condition.

9. The method of claim 1, wherein the medical device comprises a subcutaneous device.

10. The method of claim 1, wherein the sensing window is a P-wave sensing window, the first portion is a baseline portion and the second portion is a P-wave portion.

11. An implantable medical device for determining noise within response to a cardiac signal, comprising:

a plurality of electrodes sensing the cardiac signal; and a processor configured to determine a P-wave sensing window of the sensed cardiac signal, divide the P-wave sensing window into a baseline portion and a P-wave portion, determine a first derivative signal of the sensed cardiac signal within at least one of the baseline portion and the P-wave portion of the sensing window, determine a second derivative signal of the sensed cardiac signal within the at least one of the baseline portion and the P-wave of the sensing window, determine whether an amplitude of the second derivative signal satisfies an amplitude threshold, and determine noise in response to the amplitude of the second derivative signal satisfying the amplitude threshold.

12. The medical device of claim 11, wherein the first derivative signal and the second derivative signal are determined within the baseline portion of the sensing window, the processor further configured to determine positive and negative zero crossings of the first derivative signal within the baseline portion, determine whether a maximum amplitude of the second derivative signal at the positive zero crossings and a minimum amplitude of the second derivative signal at the negative zero crossings satisfy the amplitude threshold, and determine noise in response to both the maximum amplitude and the minimum amplitude satisfying the amplitude threshold.

13. The medical device of claim 11, wherein the first derivative signal and the second derivative signal are determined within the baseline portion of the sensing window, the processor further configured to determine positive and negative zero crossings of the first derivative signal within the baseline portion, determine whether a maximum amplitude of the second derivative signal at the positive zero crossings and a minimum amplitude of the second derivative signal at the negative zero crossings satisfy the amplitude threshold, and determine noise in response to only one of the maximum amplitude and the minimum amplitude satisfying the amplitude threshold.

14. The medical device of claim 11, wherein the first derivative signal and the second derivative signal are determined within the baseline portion of the sensing window, the processor further configured to determine positive and negative zero crossings of the first derivative signal within the baseline portion, determine a first number of amplitudes of the second derivative signal at the positive going zero crossing that are greater than a first amplitude threshold, determine a second number of amplitudes of the second derivative signal at the negative going zero crossing that are less than a second amplitude threshold, determine a sum of the first number of amplitudes and the second number of amplitudes, and determine noise based on the determined sum.

15. The medical device of claim 14, wherein the processor is further configured to determine whether a total number of the determined positive zero crossings and the negative zero crossings is within a zero crossings sum threshold, and determine noise in response to both the determined sum being greater than an amplitude sum threshold and the total number of the determined positive zero crossings and the negative zero crossings being within the zero crossings sum threshold.

16. The medical device of claim 11, wherein the first derivative signal and the second derivative signal are determined within the P-wave portion of the sensing window, the processor further configured to determine positive and negative zero crossings of the first derivative signal within the P-wave portion, determine whether a total number of the determined positive zero crossings and the negative zero crossing is greater than a total zero crossings threshold, and determine noise in response to the total number of the determined positive zero crossings and the negative zero crossing being greater than the total zero crossings threshold.

17. The medical device of claim 11, wherein the first derivative signal and the second derivative signal are determined within the baseline portion of the sensing window, the processor further configured to determine positive and negative zero crossings of the first derivative signal within the baseline portion, determine whether a total number of the determined positive zero crossings and the negative zero crossings is greater than a total zero crossings threshold, determine a first number of amplitudes of the second derivative signal at the positive going zero crossings of the first derivative signal that are greater than a positive going amplitude threshold, determine a second number of amplitudes of the second derivative signal at the negative going zero crossings of the first derivative signal that are less than a negative going amplitude threshold, determine whether a sum of the first number of amplitudes and the second number of amplitudes is greater than a total amplitude threshold, and determine noise in response to both the total number of the determined positive zero crossings and the negative zero crossings being greater than the total zero crossings threshold and the sum of the first number of amplitudes and the second number of amplitudes being greater than the total amplitude threshold.

18. The medical device of claim 11, wherein the processor is further configured to determine a first noise condition comprising determining whether a maximum amplitude of the second derivative signal at positive zero crossings of the first derivative signal and a minimum amplitude of the second derivative signal at negative zero crossings of the first derivative signal satisfy a first amplitude threshold, determine a second noise condition comprising determining a first number of amplitudes of the second derivative signal

at positive going zero crossings that are greater than a second amplitude threshold, and determining a second number of amplitudes of the second derivative signal at negative going zero crossings that are less than a third amplitude threshold, determine a third noise condition comprising determining a total number of positive zero crossings and negative zero crossings of the first derivative signal within the baseline portion of the sensing window, determine a fourth noise condition comprising determining a total number of positive zero crossings and negative zero crossings of the first derivative signal within the P-wave portion of the sensing window, and determine a fifth noise condition comprising determining a total number of positive zero crossings and negative zero crossings greater than a total zero crossings threshold; determining a first number of amplitudes of the second derivative signal at the positive going zero crossings of the first derivative signal that are greater than a positive going amplitude threshold; and determining a second number of amplitudes of the second derivative signal at negative going zero crossings of the first derivative signal that are less than a negative going amplitude threshold, wherein noise is determined in response to one of the first noise condition, the second noise condition, the third noise condition, the fourth noise condition and the fifth noise condition.

19. The medical device of claim 11, wherein the medical device comprises a subcutaneous device.

20. A computer-readable medium storing a set of instructions which cause a processor of an implantable medical device to perform a method of determining a noise of a cardiac signal, comprising:

- sensing the cardiac signal;
- determining a sensing window of the sensed cardiac signal, the sensing window comprising a first portion and a second portion;
- determining a first derivative signal in response to the sensed cardiac signal within only one of the first portion and the second portion of the sensing window;
- determining a second derivative signal in response to the sensed cardiac signal within the one of the first portion and the second portion of the sensing window;
- determining whether an amplitude of the second derivative signal satisfies an amplitude threshold; and
- determining noise in response to the amplitude of the second derivative signal satisfying the amplitude threshold.

21. An implantable medical device for determining noise in a cardiac signal, comprising:

- a plurality of electrodes configured to sense the cardiac signal; and
- a processor configured to determine a P-wave sensing window associated with at least one cardiac event in the sensed cardiac signal, the sensing window comprising a first portion corresponding to a baseline portion and a second portion corresponding to a P-wave portion, determine a first derivative signal of the cardiac signal within the sensing window, determine a second derivative signal of the cardiac signal within the sensing window, identify a noise event within the sensing window based at least on the analysis of amplitudes of the second derivative signal.

22. The medical device of claim 21, wherein the processor is further configured to determine positive going and negative going zero crossings in the first derivative signal within the first portion of the sensing window, determine amplitudes of the second derivative signal at the positive going and negative going zero crossings, determine a maximum

amplitude of the determined amplitudes at the positive going zero crossings, determine a minimum amplitude of the determined amplitudes at the negative going zero crossings, and identifying the noise event within the sensing window based on at least one of the maximum amplitude and the minimum amplitude.

23. The medical device of claim 22, wherein the processor is configured to identify the noise event within the sensing window when both the maximum amplitude is greater than a first threshold amplitude and the minimum amplitude is less than a second threshold amplitude.

24. The medical device of claim 23, wherein the processor is configured to identify the noise event within the sensing window when either the maximum amplitude is greater than a third threshold amplitude or the minimum amplitude is less than a fourth threshold amplitude.

25. The medical device of claim 24, wherein the third threshold is greater than the first threshold and the fourth threshold is less than the second threshold.

26. The medical device of claim 21, wherein the processor is further configured to determine positive going and negative going zero crossings in the first derivative signal within the first portion of the sensing window, determine amplitudes of the second derivative signal at the positive going and negative going zero crossings, determine a first number of the determined amplitudes of the second derivative signal at the positive going zero crossing that are greater than a fifth threshold amplitude, determine a second number of the determined amplitudes of the second derivative signal at the negative going zero crossing that are less than a sixth threshold amplitude, determine a sum of the first number of amplitudes and the second number of amplitudes, and identify the noise event within the sensing window based on the determined sum.

27. The medical device of claim 26, wherein the processor is configured to identify the noise event within the sensing window when the sum is greater than a threshold sum.

28. The medical device of any one of claim 27, wherein the processor is further configured to determine a total number of zero crossings within the first portion of the sensing window by summing the number of determined positive going and negative going zero crossings within the first portion of the sensing window, and identify the noise event within the sensing window when both the determined sum is equal to the threshold sum and the total number of zero crossings is within a predetermined range.

29. The medical device of claim 21, wherein the processor is further configured to determine positive going and negative going zero crossings in the first derivative signal within the second portion of the sensing window, determine a total number of the determined positive zero crossings and the negative zero crossings in first derivative signal of the second portion of the sensing window, and identify the noise event within the sensing window when the total number of zero crossings in first derivative signal of the second portion of the sensing window is greater than a total zero crossings threshold.

30. The medical device of claim 21, wherein the processor is further configured to determine positive going and negative going zero crossings of the first derivative signal within the first portion of the sensing window, determine a total number of the determined positive going zero crossings and the negative going zero crossings within the first portion of the sensing window, determine a first number of amplitudes of the second derivative signal at the positive going zero crossings within the first portion of the sensing window that are greater than a positive going amplitude threshold, deter-

mine a second number of amplitudes of the second derivative signal at the negative going zero crossings within the first portion of the sensing window that are less than a negative going amplitude threshold, determine whether a sum of the first number of amplitudes and the second number of amplitudes is greater than a threshold number, and identify the noise event in the sensing window when both the total number of the determined positive zero crossings and the negative zero crossings are greater than the total zero crossings threshold and the sum of the first number of amplitudes and the second number of amplitudes are greater than the threshold number.

31. The medical device of claim **21**, wherein the medical device comprises a subcutaneous device.

32. The medical device of claim **21**, wherein the baseline portion of the P-wave sensing window precedes the P-wave portion of the P-wave sensing window.

* * * * *

专利名称(译)	用于房性心律失常发作检测的方法和装置		
公开(公告)号	US9675269	公开(公告)日	2017-06-13
申请号	US14/695171	申请日	2015-04-24
[标]申请(专利权)人(译)	美敦力公司		
申请(专利权)人(译)	美敦力公司, INC.		
当前申请(专利权)人(译)	美敦力公司, INC.		
[标]发明人	SARKAR SHANTANU HANSEN DANIEL L NEITZELL GRANT A		
发明人	SARKAR, SHANTANU HANSEN, DANIEL L NEITZELL, GRANT A		
IPC分类号	A61B5/00 A61B5/0452 A61B5/046 A61N1/362 A61N1/39 A61N1/365 A61B5/0456 A61B5/04 A61B5/0464		
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优先权	62/117785 2015-02-18 US		
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外部链接	Espacenet USPTO		

摘要(译)

一种用于确定响应于心脏信号的噪声的方法和可植入医疗设备, 包括感测心脏信号, 响应于感测到的心脏信号确定感测窗口, 感测窗口包括第一部分和第二部分, 确定一阶导数信号响应于感测窗口的第一部分和第二部分中的仅一个内的感测的心脏信号, 响应于感测的第一部分和第二部分中的一个内的感测的心脏信号确定二阶导数信号窗口, 确定二阶导数信号的幅度是否满足幅度阈值, 并且响应于满足幅度阈值的二阶导数信号的幅度确定噪声。

