



US009216000B2

(12) **United States Patent**
Bechtel et al.

(10) **Patent No.:** **US 9,216,000 B2**
(45) **Date of Patent:** **Dec. 22, 2015**

(54) **LIGHT WAVELENGTH SELECTION FOR AVOIDANCE OF SURGICAL DYES**

(2013.01); *A61B 5/742* (2013.01); *A61B 5/7405* (2013.01); *A61B 5/7475* (2013.01); *A61B 19/54* (2013.01); *A61M 35/003* (2013.01)

(71) Applicant: **ViOptix, Inc.**, Fremont, CA (US)

(58) **Field of Classification Search**

(72) Inventors: **Kate LeeAnn Bechtel**, Pleasant Hill, CA (US); **Lester John Lloyd**, Orinda, CA (US)

CPC *A61B 5/1455*
USPC 600/310-344
See application file for complete search history.

(73) Assignee: **ViOptix, Inc.**, Fremont, CA (US)

(56) **References Cited**

(*) Notice: Subject to any disclaimer, the term of this patent is extended or adjusted under 35 U.S.C. 154(b) by 0 days.

U.S. PATENT DOCUMENTS

4,223,680 A 9/1980 Jobsis
5,517,987 A 5/1996 Tsuchiya

(Continued)

(21) Appl. No.: **13/887,178**

OTHER PUBLICATIONS

(22) Filed: **May 3, 2013**

Mittnacht, et al., "Methylene Blue Administration is Associated with Decreased Cerebral Oximetry Values," *Anesthesia & Analgesia*, Aug. 2008, vol. 105, No. 2, pp. 549-550.

(65) **Prior Publication Data**

US 2014/0155716 A1 Jun. 5, 2014

Primary Examiner — Tse Chen

Assistant Examiner — Marjan Fardanesh

Related U.S. Application Data

(60) Provisional application No. 61/642,399, filed on May 3, 2012, provisional application No. 61/642,395, filed on May 3, 2012, provisional application No. 61/642,393, filed on May 3, 2012, provisional application No. 61/642,389, filed on May 3, 2012, provisional application No. 61/682,146, filed on Aug. 10, 2012.

(74) *Attorney, Agent, or Firm* — Aka Chan LLP

(51) **Int. Cl.**

A61B 5/1455 (2006.01)
A61B 5/00 (2006.01)
A61B 5/1495 (2006.01)
A61B 19/00 (2006.01)
A61M 35/00 (2006.01)

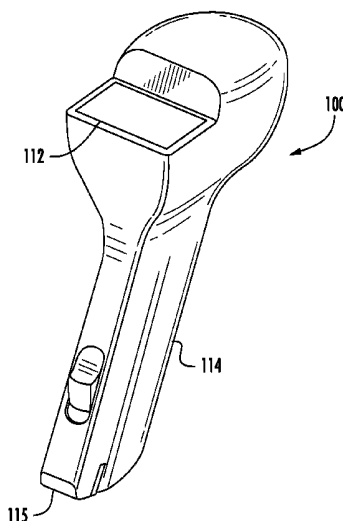
(57) **ABSTRACT**

A tissue oximetry device utilizes at least three or at least four different wavelengths of light for collection of reflectance data where the different wavelengths are longer than 730 nanometers. The three or four wavelengths are utilized to generate a range of reflectance data suited for accurate determination of oxygenated hemoglobin and deoxygenated hemoglobin concentrations. The relatively long wavelengths decrease optical interference from certain dyes, particularly methylene blue and PVPI, which may be present on tissue being analyzed for viability and further enhance the generation of accurate reflectance data. The wavelengths are 760 nanometers, 810 nanometers, and 850 nanometers, or 760 nanometers, 810 nanometers, 850 nanometers, and 900 nanometers.

(52) **U.S. Cl.**

CPC *A61B 5/74* (2013.01); *A61B 5/0075* (2013.01); *A61B 5/1455* (2013.01); *A61B 5/1495* (2013.01); *A61B 5/14551* (2013.01); *A61B 5/14552* (2013.01); *A61B 5/7282*

33 Claims, 5 Drawing Sheets



(56)

References Cited

U.S. PATENT DOCUMENTS

6,587,701 B1 *	7/2003	Stranc et al.	600/310	6,735,458 B2 *	5/2004	Cheng et al.	600/323
6,597,931 B1 *	7/2003	Cheng et al.	600/310	2008/0139908 A1	6/2008	Kurth	
				2009/0234209 A1	9/2009	Lash et al.	
				2011/0237911 A1 *	9/2011	Lamego et al.	600/323

* cited by examiner

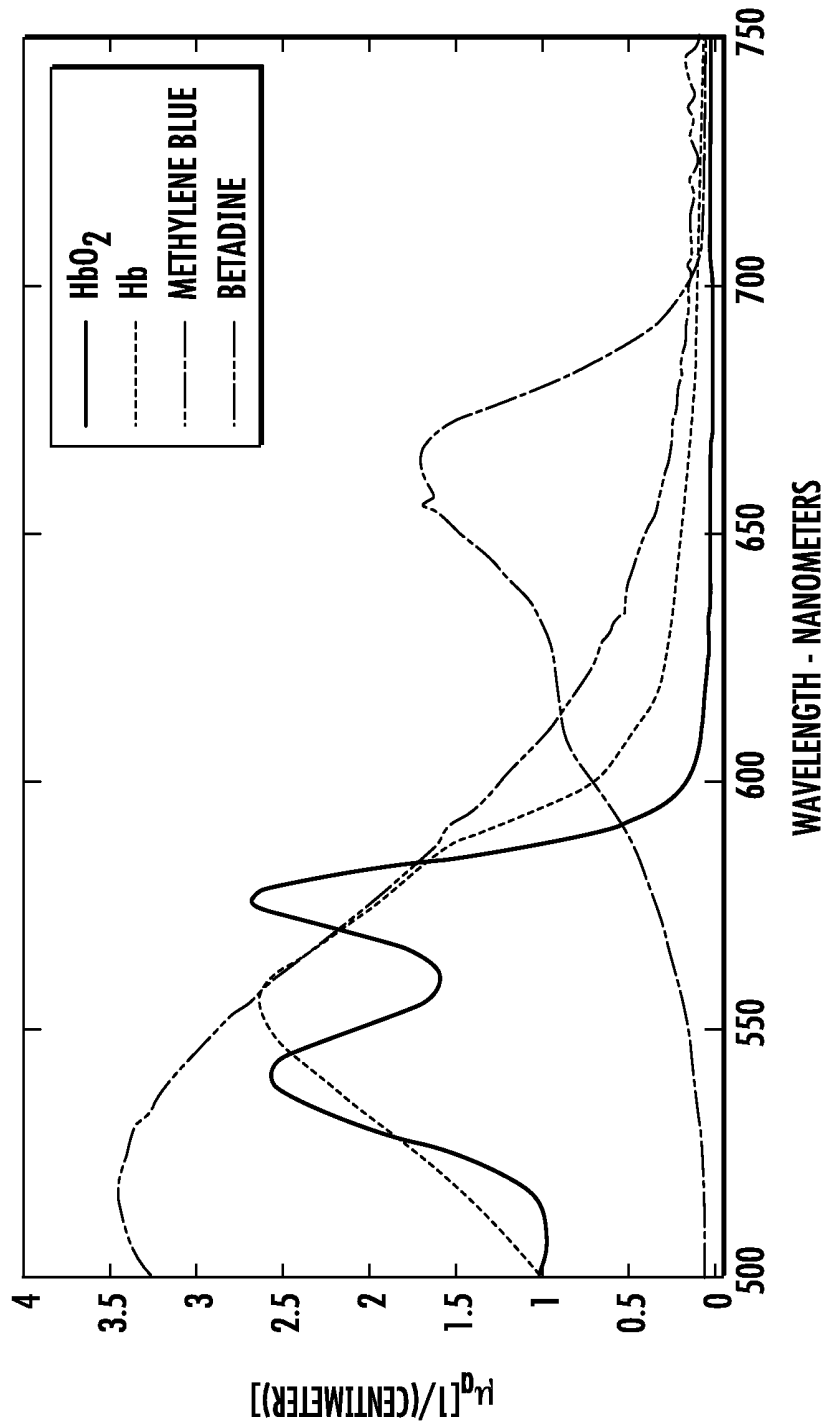


FIG. 1

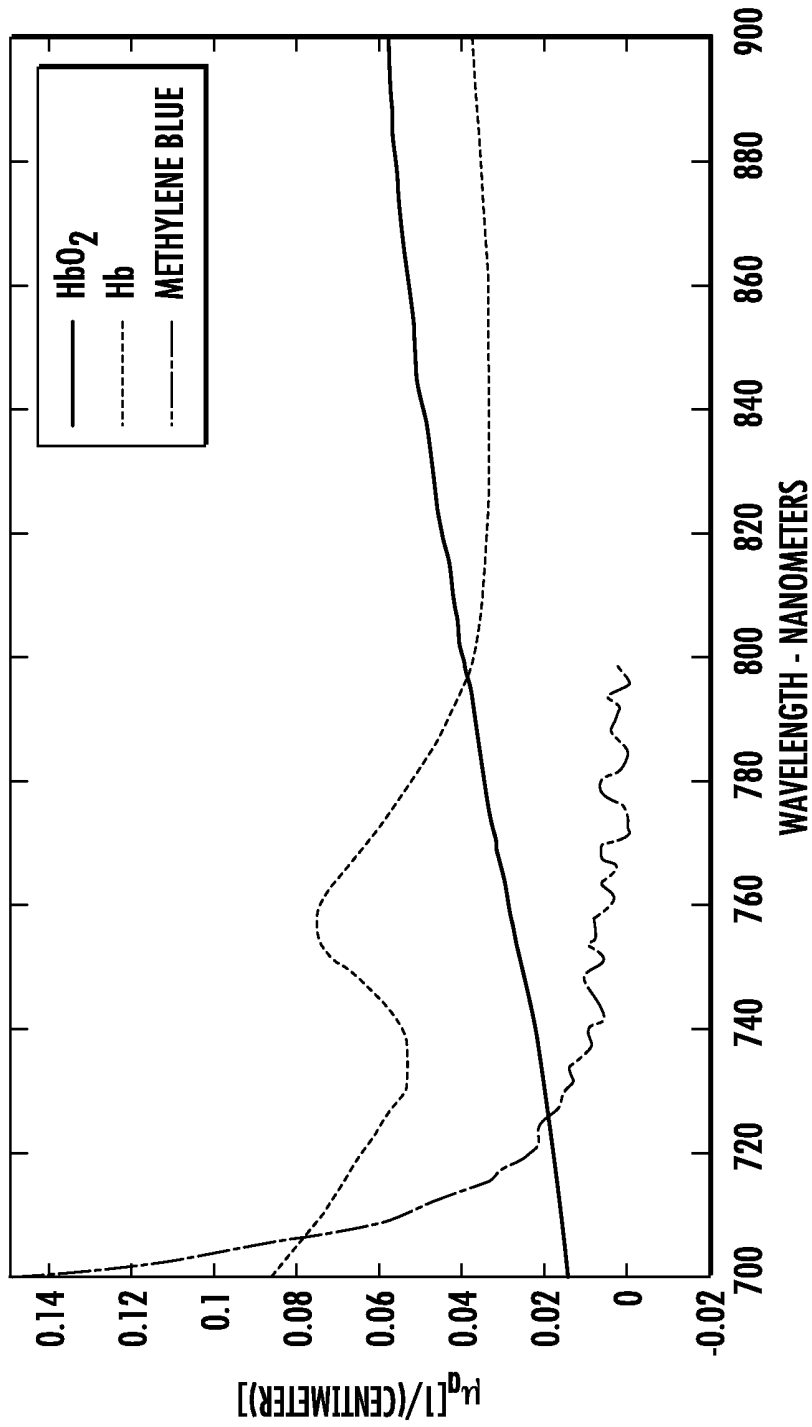


FIG. 2

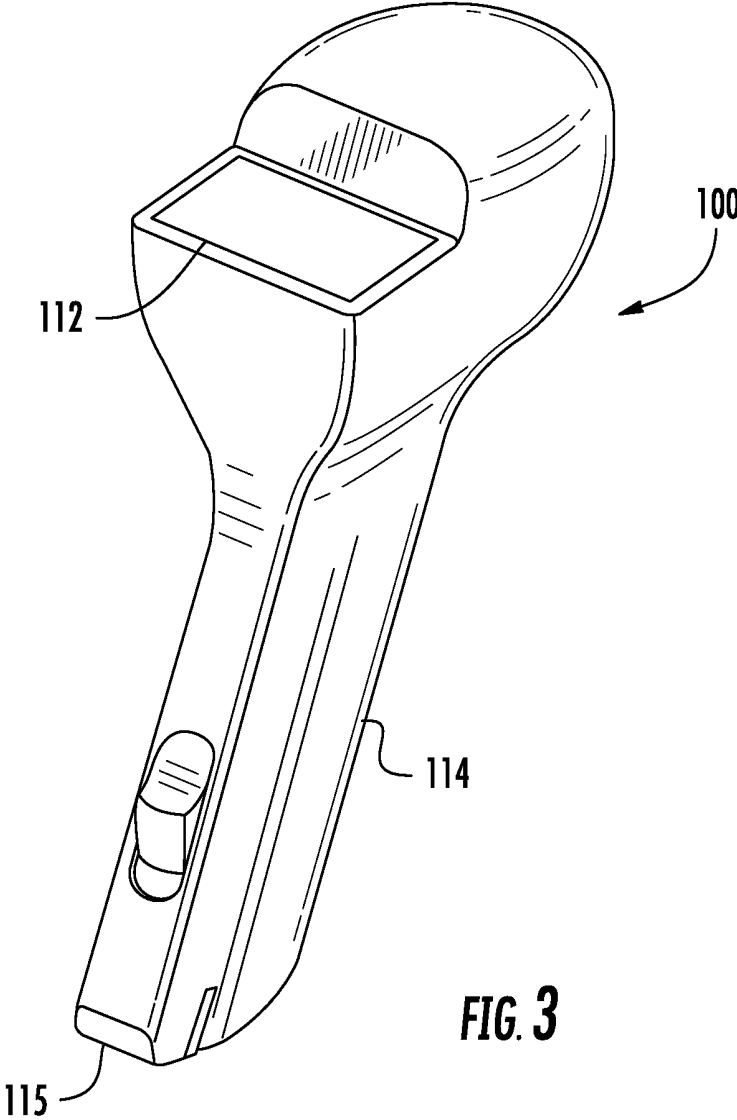
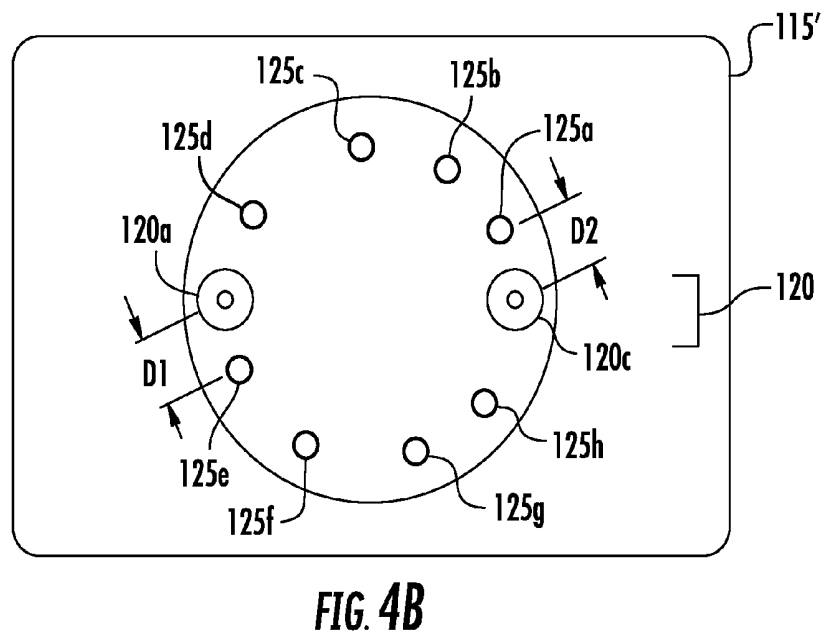
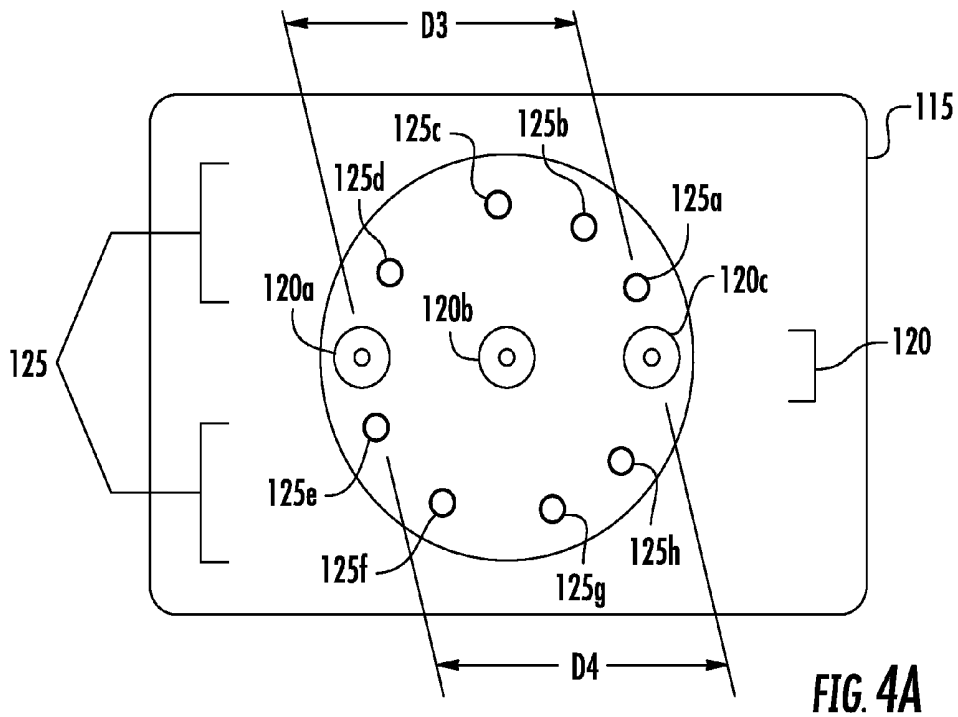


FIG. 3



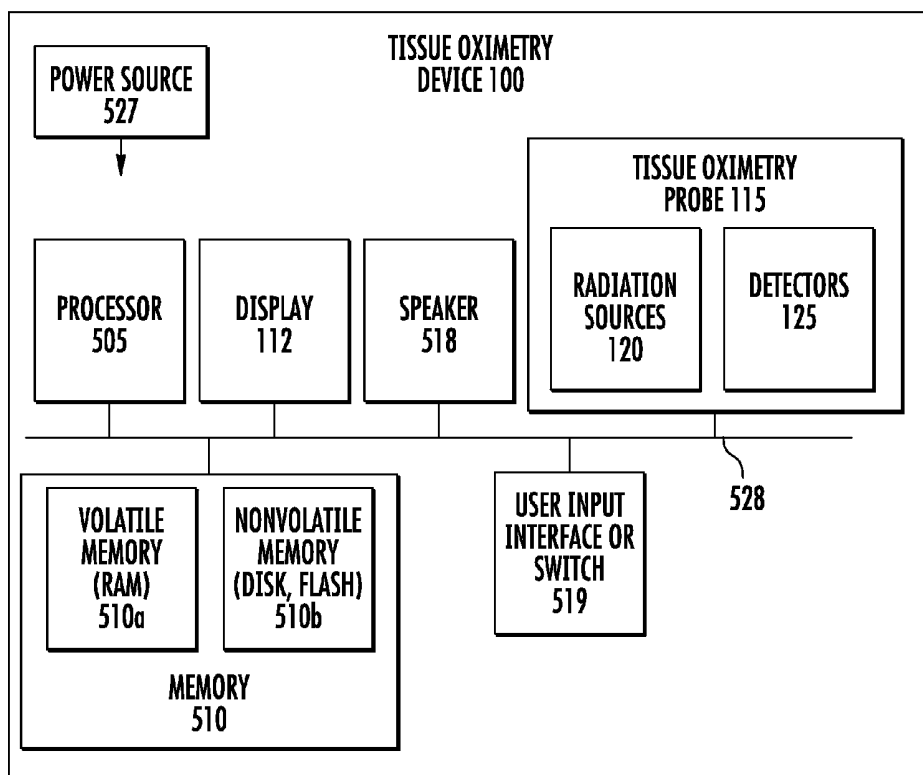


FIG. 5

LIGHT WAVELENGTH SELECTION FOR AVOIDANCE OF SURGICAL DYES

CROSS-REFERENCE TO RELATED APPLICATIONS

This patent application claims the benefit of U.S. provisional patent applications 61/642,389, 61/642,393, 61/642,395, and 61/642,399, filed May 3, 2012, and 61/682,146, filed Aug. 10, 2012, which are incorporated by reference along with all other references cited in this application.

BACKGROUND OF THE INVENTION

The present invention relates generally to optical systems that monitor oxygen levels in tissue. More specifically, the present invention relates to optical probes that include sources and detectors on sensor heads of the optical probes for emitting and detecting light.

Oximeters are medical devices used to measure oxygen saturation of tissue in humans and living things for various purposes. For example, oximeters are used for medical and diagnostic purposes in hospitals and other medical facilities (e.g., surgery, patient monitoring, or ambulance or other mobile monitoring for, e.g., hypoxia); sports and athletics purposes at a sports arena (e.g., professional athlete monitoring); personal or at-home monitoring of individuals (e.g., general health monitoring, or personal training for a marathon); and veterinary purposes (e.g., animal monitoring).

Pulse oximeters and tissue oximeters are two types of oximeters that operate on different principles. A pulse oximeter requires a pulse in order to function. A pulse oximeter typically measures the absorbance of light due to the pulsing arterial blood. In contrast, a tissue oximeter does not require a pulse in order to function, and can be used to make oxygen saturation measurements of a tissue flap that has been disconnected from a blood supply.

Human tissue, as an example, includes a variety of molecules that can interact with light via scattering or absorption (e.g., via light-absorbing chromophores). Such chromophores include oxygenated and deoxygenated hemoglobins, melanin, water, lipid, and cytochrome. Oxygenated and deoxygenated hemoglobins are the most dominant chromophores in the spectrum range of 600 nanometers to 900 nanometers. Light absorption differs significantly for oxygenated and deoxygenated hemoglobins at certain wavelengths of light. Tissue oximeters can measure oxygen levels in human tissue by exploiting these light-absorption differences.

Despite the success of existing oximeters, there is a continuing desire to improve oximeters by, for example, improving measurement accuracy; reducing measurement time; lowering cost; reducing size, weight, or form factor; reducing power consumption; and for other reasons, and any combination of these.

In particular, assessing a patient's oxygenation state is important as it is an indicator of the state of the patient's health. Thus, oximeters are often used in clinical settings, such as during surgery and recovery, where it may be suspected that the patient's tissue oxygenation state is unstable. For example, during surgery, oximeters should be able to quickly deliver accurate oxygen saturation measurements under a variety of non-ideal conditions. While existing oximeters have been sufficient for post-operative tissue monitoring where speed of measurement is less critical, existing oximeters fluctuate substantially and give inaccurate saturation measurements when used during surgery where various

elements can interfere with accurate reading, such as if the oximeter comes in contact with blood.

Therefore, there is a need for improved tissue oximetry probes and methods of making measurements using these probes.

BRIEF SUMMARY OF THE INVENTION

A tissue oximetry device utilizes at least two different wavelengths of light for collection of reflectance data where the wavelengths are above 700 nanometers. Utilizing two, three, or four wavelengths generates a range of data that is suited for accurate determination of oxygenated hemoglobin and deoxygenated hemoglobin concentrations.

According to one embodiment, a tissue oximetry device includes a processor; a memory coupled to the processor; and a plurality of light sources. The light sources are controlled by the processor, and generate and emit at least two wavelengths of light longer than 700 nanometers. The tissue oximetry device further includes a plurality of detectors configured to be controlled by the processor. The processor is configured to: control the plurality of light sources to generate and emit the light into tissue, control the plurality of detectors to detect the light subsequent to reflection of the light from the tissue, control the plurality of detectors to generate reflectance data for the tissue based on detection of the light by the plurality of detectors, and determine the oxygen saturation for the tissue based on the reflectance data.

According to one specific embodiment, the at least two wavelengths are approximately 760 nanometers and 850 nanometers. According to an alternative specific embodiment, the plurality of light sources is configured to generate and emit at least three wavelengths of light having wavelengths of 760 nanometers, 810 nanometers, and 850 nanometers. According to another alternative specific embodiment, the plurality of light sources is configured to generate and emit at least four wavelengths of light having wavelengths of approximately 760 nanometers, 810 nanometers, 850 nanometers, and 900 nanometers.

According to another embodiment, a tissue oximetry device includes a processor; a memory coupled to the processor; and a plurality of light sources that are controlled by the processor. The light sources are configured to generate and emit at least two wavelengths of light that are longer than wavelengths of primary absorption peaks of methylene blue. The tissue oximetry device further includes a plurality of detectors configured to be controlled by the processor. The processor is configured to: control the plurality of light sources to generate and emit the light into tissue; control the plurality of detectors to detect the light subsequent to reflection of the light from the tissue; control the plurality of detectors to generate reflectance data for the tissue based on detection of the light by the plurality of detectors; and determine the oxygen saturation for the tissue based on the reflectance data.

These relatively long wavelengths tend to decrease optical interference with certain dyes, particularly methylene blue and povidone-iodine (PVPI, e.g., Betadine® of Purdue Products L.P. of Stamford, Conn.), which may be present in tissue being analyzed for viability, and further enhances the generation of accurate reflectance data. The wavelengths also avoid gentian violet, which is often used in tissue marking pens. The wavelengths utilized by the tissue oximetry device are outside of the peak absorptive ranges of methylene blue, gentian violet, and PVPI. Therefore, relatively accurate reflectance data may be acquired in an increased number of surgical situations than was acquired by tissue oximetry device utiliz-

ing other wavelengths. Further, the use of these particular two, three, or four different wavelengths provides sufficient reflectance data to solve the two-variable, three-variable, or four-variable relations from which oxygenated hemoglobin and deoxygenated hemoglobin concentrations can be determined, depending on how many additional tissue chromophores are included (e.g., melanin, or others). The utilization of optimal probing wavelengths improves tissue oximetry device performance in intraoperative situations involving dyes as compared to the tissue oximetry devices considered to be prior art.

Other objects, features, and advantages of the present invention will become apparent upon consideration of the following detailed description and the accompanying drawings, in which like reference designations represent like features throughout the figures.

BRIEF DESCRIPTION OF THE DRAWINGS

FIG. 1 is an absorption graph that shows the absorption coefficient of methylene blue and PVPI at wavelengths ranging from 500 nanometers to just below 750 nanometers and shows the predominant absorption of wavelengths below 700 nanometers for methylene blue.

FIG. 2 is an absorption graph that shows the absorption coefficient of methylene blue at wavelengths ranging from 700 nanometers to 900 nanometers.

FIG. 3 is a simplified image of a tissue oximetry device according to one embodiment.

FIG. 4A is a simplified end view of the tissue oximetry probe according to one embodiment.

FIG. 4B is a simplified end view of the tissue oximetry probe according to an alternative embodiment.

FIG. 5 is a block diagram of the tissue oximetry device according to one embodiment.

DETAILED DESCRIPTION OF THE INVENTION

Colored dyes often are present on or have been absorbed by the tissue regions that clinicians wish to check for viability. Methylene blue is one dye that is often used for sentinel lymph node biopsies, which are often performed during the same surgical session as a mastectomy in order to determine the degree to which cancerous tissue may have spread. Therefore, methylene blue can be present in the tissue being analyzed for viability for reconstruction or the like. Methylene blue absorbs light readily in the 500 nanometer to 700 nanometer range with the absorption tailing off at about 730 nm.

Povidone-iodine (PVPI, e.g., Betadine® of Purdue Products L.P. of Stamford, Conn.) is an orange dye that is often used as an antiseptic prior to making surgical incisions and may therefore also be present on tissue of interest. Similar to methylene blue, PVPI absorbs light readily in the 500 nanometer to 700 nanometer range, however to a lesser degree than methylene blue. Further, gentian violet is a dye that is often used in tissue marking pens, such as the pens used by plastic surgeons and may therefore be present on tissue of interest.

FIGS. 1 and 2 are absorption graphs that show the absorption coefficient μ_a of methylene blue at wavelengths ranging from 500 nanometers to 900 nanometers. FIG. 1 also shows the predominant absorption by methylene blue of wavelengths below 700 nanometers and shows the primary absorption peaks of methylene blue centered at about 600 nanometers and 660 nanometers. FIG. 1 also shows the absorption coefficient μ_a of PVPI at wavelengths ranging from 500 nanometers to just below 750 nanometers. FIG. 1 also shows the predominant absorption by PVPI of wavelengths below

650 nanometers and shows the primary absorption peak of PVPI centered at about 510 nanometers.

The presence of methylene blue, PVPI, or other dyes can interfere with the determinations of tissue viability. For example, surgeons may use tissue oximetry devices for determining the viability of tissue, and dyes present on the tissue can absorb the wavelengths used by the tissue oximetry devices for providing tissue viability information.

FIG. 3 is a simplified image of a tissue oximetry device **100** according to one embodiment. Tissue oximetry device **100** is configured to make tissue oximetry measurements, such as intraoperatively and postoperatively. In an implementation, the tissue oximetry device is handheld and can make tissue oximetry measurements and display these measurements, without needing to connect to another external component either via a cable or wirelessly. The electronics to make measurements and calculations is contained entirely within the housing of the tissue oximetry device. The tissue oximetry device is a standalone handheld tissue oximeter device, without a cable or wireless connection.

Tissue oximetry device **100** may be a handheld device that includes a tissue oximetry probe **115** (also sometimes referred to as a sensor head), which may be positioned at an end of a sensing arm **114**. Tissue oximetry device **100** is configured to measure the oxygen saturation of tissue by emitting light, such as red and near-infrared light, from tissue oximetry probe **115** into tissue, and collecting light reflected from the tissue at the tissue oximetry probe.

Tissue oximetry device **100** may include a display **112** or other notification device that notifies a user of oxygen saturation measurements made by the tissue oximetry device. While tissue oximetry probe **115** is described as being configured for use with tissue oximetry device **100**, which is a handheld device, tissue oximetry probe **115** may be used with other tissue oximetry devices, such as a modular tissue oximetry device where the tissue oximetry probe is at the end of a cable device that connects to a base unit. The cable device might be a disposable device that is configured for use with a single patient and the base unit might be a device that is configured for repeated use. Such modular tissue oximetry devices are well understood by those of skill in the art and are not described further.

FIG. 4A is a simplified end view of tissue oximetry probe **115** according to one embodiment. Tissue oximetry probe **115** is configured to contact tissue (e.g., a patient's skin) for which a tissue oximetry measurement is to be made. Tissue oximetry probe **115** includes a set of light sources **120** (generally light sources **120**) and includes a set of detectors **125** (generally detectors **125**). The set of light sources **120** may include two or more light sources. According to the embodiment shown in FIG. 4A, tissue oximetry probe **115** includes three light sources **120a**, **120b**, and **120c**, but may alternatively include two light sources, such as light sources **120a** and **120c** where light source **120b** is omitted. Additional light sources (not shown) can be added. FIG. 4B is a simplified end view of a tissue oximetry probe **115'** according to an embodiment where the tissue oximetry probe includes the two light sources **120a** and **120c**, but does not include light source **120b**. Aside from the different number of light sources, tissue oximetry probes **115** and **115'** are substantially similar.

The set of detectors **125** may include eight detectors **125a**, **125b**, **125c**, **125d**, **125e**, **125f**, **125g**, and **125h** as shown, but may include more or fewer detectors. Detectors **125** are positioned with respect to outer light sources **120a** and **120c** such that eight or more (e.g., fourteen) unique source-to-detector distances are created. The shortest source-to-detector distances may be the same. For example, the shortest source-to-

detector distance D1 between light source **120a** and detector **125e**, and the shortest source-to-detector distance D2 between light source **120c** and detector **125a** may be the same. It follows that the source-to-detector distance D3 between light source **120a** and detector **125a**, and the source-to-detector distance D4 between light source **120c** and detector **125e** may also be the same. The source-to-detector distances D3 and D4 are the longest source-to-detector distance for light sources **120a** and **120c**. With the exception of the shortest source-to-detector distance and the longest source-to-detector distance for light sources **120a** and **120c**, the source-to-detector distances for light sources **120a** and **120c** may be unique. As described above, tissue oximetry probe **115** may have fourteen unique source-to-detector distances that allow for fourteen reflectance data points to be collected by detectors **125** from each wavelength of light emitted from light sources **120**. As described in further detail below, each light source **120** is configured to generate and emit a number of wavelengths.

Detectors **125** are solid state detectors and may be mounted on a printed circuit board (PCB, not shown), which routes various signal to and from the detectors. Further, detectors **125** may be combined devices or discrete devices.

While the tissue oximetry probes **115** and **115'** are described above as having circularly arranged detectors, the detectors may be positioned in other arrangements, such as linear, triangular, rectangular, square, and others. In some embodiments, the light sources may also be alternatively arranged, such as in a triangular arrangement, a rectangular arrangement, and others.

In a specific implementation, detectors **125** are positioned with respect to outer light sources **120a** and **120c** such that four or more (e.g., fourteen) unique source-to-detector distances are created. With greater numbers of source-to-detector distances, this can be used to obtain greater accuracy, faster calibration, and redundancy (when duplicate source-to-detector distances are provided). At least two source-to-detector distances are about 1.5 millimeters or less (e.g., 0.5 millimeters up to about 1.7 millimeters), and at least two more two source-to-detectors distances are about 2.5 millimeters or greater (e.g., 1.5 millimeters up to about 3.2 millimeters).

In other words, a first source-to-detector distance is about 1.5 millimeters or less. A second source-to-detector distance is about 1.5 millimeters or less. A third source-to-detector distance is about 2.5 millimeters or greater. A fourth source-to-detector distance is about 2.5 millimeters or greater. There can be various numbers of sources and detector arrangements to obtain these four source-to-detector distances, such as one source and four detectors, two sources and two detectors, one detector and four sources, or other arrangements and combinations.

For example, an implementation includes at least two sources and at least two detectors, where a maximum distance between a source and a detector is about 4 millimeters (or about 5 millimeters). At least two source-to-detector are about 2.5 millimeters or greater. At least two source-to-detector distances are about 1.5 millimeters or less.

When a greater number of sources and detectors are used, greater numbers of source-to-detector distances are available. As discussed, these can be used to provide greater accuracy, faster calibration, or redundancy, or a combination. The arrangement of the sources and detectors can be in circular pattern, such as at points along the arc of a circle with radius (e.g., 4 millimeters, or 5 millimeters). In an implementation, a tolerance of the detector or source positions on the arc is within 10 microns of the arc curve. In other implementations, the tolerance is within about 0.5 millimeters.

Wavelengths Generated and Emitted from the Light Sources

Each light source **120** may include a fiber optic cable and one or more light emitting diodes (LEDs) or laser diodes (generally wavelength sources) that transmit generated light into the fiber optic cable. For example, each light source **120** may include two or more wavelength sources that generate two or more substantially unique wavelengths. The wavelengths may all be longer than 730 nanometers, e.g., in the red and near infrared.

According to an embodiment where each light source **120** includes two wavelength sources, the wavelength sources may be configured to generate and emit wavelengths of approximately 760 nanometers (e.g., ± 10 nanometers), and 850 nanometers (e.g., ± 20 nanometers). According to an embodiment where each light source **120** includes three wavelength sources, the wavelength sources may be configured to generate and emit wavelengths of approximately 760 nanometers (e.g., ± 10 nanometers), 810 nanometers (e.g., ± 10 nanometers), and 850 nanometers (e.g., ± 20 nanometers). According to another embodiment, where each light source **120** includes four wavelength sources, the wavelength sources may be configured to emit wavelengths of approximately 760 nanometers (e.g., ± 10 nanometers), 810 nanometers (e.g., ± 10 nanometers), 850 nanometers (e.g., ± 20 nanometers), and 900 nanometers (e.g., ± 20 nanometers). Additional and/or alternative wavelengths may be utilized by tissue oximetry device **100**.

Use of the described wavelengths by tissue oximetry device **100** tends to decrease the fraction of emitted light that can be absorbed by methylene blue, gentian violet, and PVPI, and thereby increases the fraction of light that can be scattered or absorbed by intrinsic tissue elements and generates accurate reflectance data. Accurate reflectance data is necessary in order to extract the optical properties of tissue from which the concentrations of oxygenated and deoxygenated hemoglobin can be derived.

For the foregoing described wavelengths, tissue scattering is relatively low and light penetrates farther into tissue than shorter wavelengths. Further, the foregoing described wavelengths are on both sides of an oxygenated-deoxygenated hemoglobin spectral crossing point called an isosbestic point, which is 810 nanometers for hemoglobin. As such, when one chromophore (e.g., oxygenated hemoglobin) has high absorption, the other chromophore (e.g., deoxygenated hemoglobin) then has low absorption and vice versa. The tissue oximetry device's utilization of wavelengths surrounding the isosbestic point provides for relatively improved statistics for oxygen saturation determinations.

In at least one of the foregoing described embodiments, tissue oximetry device **100** utilizes a wavelength at approximately the isosbestic point, at 810 nanometers. At the isosbestic point the absorption of the 810 nanometer wavelength for oxygenated hemoglobin and deoxygenated hemoglobin are equivalent and therefore provides a stable reference point in the reflectance data generated by detectors **125**. Relatively longer wavelengths, such as the 900 nanometer wavelength of at least one embodiment allows for distinguishing between the absorption curve for deoxygenated hemoglobin from the absorption curve for melanin.

Tissue Oximetry Device Circuit

FIG. 5 is a block diagram of tissue oximetry device **100** according to one embodiment. Tissue oximetry device **100** according to the embodiment shown in FIG. 5 includes display **112**, a processor **505**, a memory **510**, a speaker **518**, one or more user-selection devices **519** (e.g., one or more switches for initiating oxygen saturation measurements), the

set of light sources **120**, the set of detectors **125**, and a power source (e.g., a battery) **527**. The foregoing listed components may be linked together via a bus **528**, which may be the system bus architecture of tissue oximetry device **100**. Although this figure shows one bus that connects to each component, the busing is illustrative of any interconnection scheme serving to link these components or other components included in tissue oximetry device **100** subsystems. For example, speaker **518** (e.g., an alternative device for notifying a user of oxygen saturation measurements) could be connected to a subsystem through a port or have an internal direct connection to processor **516**. Further, the components described are housed in a mobile housing (see FIG. 1) of tissue oximetry device **100** according to at least one embodiment.

Processor **505** may include a microprocessor, a microcontroller, control logic, a multi-core processor, or the like. Further, processor **505** may control turning on and turning off the wavelength sources as described below. Memory **510** may include a variety of memories, such as a volatile memory **510a** (e.g., a RAM), a nonvolatile memory **519b** (e.g., a disk, Flash memory, electrically erasable memory, PROM, and others). Memory **510** may collect and store reflectance data generated by detectors **125**. Different implementations of tissue oximetry device **100** may include any number of the listed components, in any combination or configuration, and may also include other components not shown.

Power source **127** can be a battery, such as a disposable battery. Disposable batteries are discarded after their stored charge is expended. Some disposable battery chemistry technologies include alkaline, zinc carbon, or silver oxide. The battery has sufficient stored charge to allow use of the handheld device for several hours. After use, the handheld unit is discarded.

In other implementations, the battery can also be rechargeable where the battery can be recharged multiple times after the stored charge is expended. Some rechargeable battery chemistry technologies include nickel cadmium (NiCd), nickel metal hydride (NiMH), lithium ion (Li-ion), and zinc air. The battery can be recharged, for example, via an AC adapter with cord that connects to the handheld unit. The circuitry in the handheld unit can include a recharger circuit (not shown). Batteries with rechargeable battery chemistry may be sometimes used as disposable batteries, where the batteries are not recharged but disposed of after use.

Use of Wavelengths for Optical Probing.

Oxygenated and deoxygenated hemoglobin concentrations, from which oxygen saturation can be calculated, can be related to the absorption coefficient μ_a of a region of tissue for a given wavelength of light. In some cases, a simple relationship is used for calculation where the absorption coefficient is assumed to depend only on the concentrations of oxygenated and deoxygenated hemoglobin. However, melanin and water present in tissue can also absorb incident light so this simple relationship may be insufficient for highly accurate concentration calculations, as absorption from water and melanin may be incorrectly attributed to oxygenated or deoxygenated hemoglobin. A relationship between the absorption coefficient and the concentrations of oxygenated hemoglobin (HbO₂), deoxygenated hemoglobin (Hb), water (H₂O), and melanin (mel) may be:

$$\mu_a = 2.303(\epsilon_{HbO_2}[HbO_2] + \epsilon_{Hb}[Hb] + \epsilon_{H_2O}[H_2O] + \epsilon_{mel}[mel])$$

where $\epsilon_{species}$ denotes the molar absorptivity of a given species and bracketed quantities indicate concentration values.

The shape of a reflectance curve (generated by plotting the intensity of diffusely reflected or re-emitted light) can be analyzed to obtain the absorption and scattering coefficients for a given region of tissue. There are four unknown concentrations (i.e., [HbO₂], [Hb], [H₂O], and [mel]) in the above relationship that correspond to the absorption coefficient. Once the absorption coefficient is determined for a given wavelength, the relationship becomes an equation of four unknown variables. However, since the concentrations of oxygenated and deoxygenated hemoglobin, water, and melanin should not vary considerably over the course of a probe measurement, probing the tissue with four different wavelengths emitted by the wavelength sources can provide four values for μ_a , which can be used to determine the four relevant concentrations in the expression for μ_a . That is, a system of four equations with four unknown variables can be solved, as is well understood. From the determined concentrations of oxygenated hemoglobins [HbO₂] and deoxygenated hemoglobins [Hb], the oxygen saturation of tissue can be determined.

According to the embodiment where three wavelengths are emitted by the wavelength sources, the contributions from water, melanin, and other light absorbers can be combined into a single term and expressed as:

$$\mu_a = 2.303(\epsilon_{HbO_2}[HbO_2] + \epsilon_{Hb}[Hb] + \epsilon_{H_2O, mel}[H_2O, mel]).$$

If three absorption coefficients μ_a are determined for the three wavelengths, then the three relevant concentrations for [HbO₂], [Hb], and [H₂O, mel]) can be determined, and the oxygen saturation can again be determined from the determined concentrations of oxygenated and deoxygenated hemoglobins. The absorption coefficients may be determined from the reflectance data by a variety of methods, such as fitting the reflectance data to one or more predetermined reflectance curves, where each predetermined reflectance curve represents a unique absorption coefficient. The absorption coefficients may alternatively be determined by vector multiplication with the net analyte signal, which is described in U.S. Pat. No. 6,597,931, titled "System and Method for Absolute Oxygen Saturation," and is incorporated by reference.

Wavelength Source Control

The wavelength sources may be cycled on and off at a variety of frequencies. For example, the wavelength sources may be turned on in sequence with one wavelength source on at any one time. The wavelength sources may be cycled at 30 hertz. Additionally each wavelength source may be modulated at a variety of frequencies in order to reject ambient light. For example, each wavelength source may be individually modulated at 2.5 kilohertz. Further, the wavelength sources may be individually cycled in a specific order. Detectors **125** may be substantially continuously monitored as the wavelength sources are cycled. Processor **505** may control the cycle order of the wavelength sources. Based on the cycle order, the reflectance data collected by detectors **125** may be appropriately categorized according to wavelength based on the known cycling of the wavelength sources on and off. The reflectance data may be stored in memory **510** for use by processor **505** in determining the oxygenated and deoxygenated hemoglobin concentrations and to further determine the oxygen saturation of tissue being probed.

This description of the invention has been presented for the purposes of illustration and description. It is not intended to be exhaustive or to limit the invention to the precise form described, and many modifications and variations are possible in light of the teaching above. The embodiments were

chosen and described in order to best explain the principles of the invention and its practical applications. This description will enable others skilled in the art to best utilize and practice the invention in various embodiments and with various modifications as are suited to a particular use. The scope of the invention is defined by the following claims. 5

The invention claimed is:

1. A handheld tissue oximetry device comprising:

a housing comprising; 10

a processor contained within the housing;

a memory, contained within the housing, wherein the memory is coupled to the processor;

a display, coupled to the processor, wherein the display is visible from an exterior of the housing; 15

a battery, contained within the housing, coupled to and supplies power to the processor, memory, and display; and

a tip portion of the housing;

a sensor module, coupled to the processor, wherein the sensor module comprises a probe face that is retained by the tip portion of the housing at a relatively fixed position with respect to the housing and that is placed against and faces tissue to be measured, and the sensor module comprises: 25

a first plurality of detector structures, formed on the probe face, arranged in a circular arrangement, symmetrically about a point on a line intersecting a circle of the circular arrangement at a first point and a second point; 30

a second plurality of detector structures, formed on the probe face, arranged asymmetrically about the point on the line in the circular arrangement;

a first source structure, formed on the probe face, positioned at the first point of the circle of the circular arrangement; 35

a second source structure, formed on the probe face, positioned at the second point of the circle of the circular arrangement;

a first source diode and a second source diode adapted to emit radiation having at least four wavelengths longer than 730 nanometers; 40

a first optical fiber optically coupled between the first source diode and the first source structure;

a second optical fiber optically coupled between the second source diode and the second source structure, wherein the first optical fiber transmits radiation emitted by the first source diode to the first source structure, and the second optical fiber transmits radiation emitted by the second source diode to the second source structure; 50

a first detector structure on the circle of the first plurality of detector structures, wherein a first distance is from the first detector structure to the first source structure, a second distance is from the first detector structure to the second source structure, and the first distance is greater than the second distance; 55

a second detector structure on the circle of the first plurality of detector structures, arranged symmetrically with respect to the first detector structure about the point on the line, wherein a third distance is from the second detector structure to the first source structure, a fourth distance is from the second detector structure to the second source structure, and the fourth distance is greater than the third distance; 60

the first distance is the same as the fourth distance, and the second distance is the same as the third distance; 65

a third detector structure on the circle of the second plurality of detector structures, arranged asymmetrically with respect to the first plurality of detector structures about the point on the line, wherein a fifth distance is from the third detector structure to the first source structure, a sixth distance is from the third detector structure to the second source structure, the fifth distance is different from the first distance and the second distance, and the sixth distance is different from the first distance and the second distance; and

a fourth detector structure on the circle of the second plurality of detector structures, arranged asymmetrically with respect to the first plurality of detector structures and the third detector structure about the point on the line, wherein a seventh distance is from the fourth detector structure to the first source structure, an eighth distance is from the fourth detector structure to the second source structure, the seventh distance is different from the first, second, fifth, and sixth distances, and the eighth distance is different from the first, second, fifth, and sixth distances, wherein the first distance is greater the fifth, sixth, seventh, and eighth distances, and the second distance is less than the fifth, sixth, seventh, and eighth distances, and

wherein the processor is adapted to:

control the first and second diodes to emit the radiation at the four wavelengths to the first and second source structures via the first and second optical fibers and to emit the radiation at the four wavelengths into tissue to be measured from the first and second source structures,

control the first and second plurality of detector structures to detect the radiation at the four wavelengths subsequent to reflection of the radiation from the tissue to be measured,

receive digital reflectance data for the detected radiation detected by the first and second plurality of detector structures,

calculate a plurality of absorption coefficients using the digital reflectance data for the radiation at the four wavelengths,

solve a set of reflection coefficient equations for the tissue to be measured using the plurality of absorption coefficients to determine concentration values of oxygenated hemoglobin, deoxygenated hemoglobin, water, and melanin for the tissue, wherein the concentration values of oxygenated hemoglobin and deoxygenated hemoglobin are relatively independent of the concentration values of water and melanin for the tissue, and

determine the absolute oxygen saturation for the tissue using the concentration values of oxygenated hemoglobin and deoxygenated hemoglobin.

2. The handheld tissue oximetry device of claim **1** wherein at least two of the four wavelengths are approximately 760 nanometers and 850 nanometers.

3. The handheld tissue oximetry device of claim **1** wherein the processor is adapted output from the display a value indicative of the absolute oxygen saturation value for the tissue to be measured.

4. The handheld tissue oximetry device of claim **1** wherein a ninth distance is from the first source structure to the second source structure, and the ninth distance is greater than the first, second, third, fourth, fifth, sixth, seventh, and eighth distances.

5. The handheld tissue oximetry device of claim **1** wherein at least three of the wavelengths are approximately 760 nanometers, 810 nanometers, and 850 nanometers.

6. The handheld tissue oximetry device of claim 1 wherein the handheld tissue oximetry device is a standalone unit, when the handheld tissue oximetry device is used, the housing comprising the processor, memory, display, and battery of the device is cradled on the purlicue between a thumb and forefinger of a hand of a user while the display is at a proximal end of the device and the tip portion of the housing extends in a distal direction to a distal end of the device, and

while the device is in the user's hand, the user positions the probe face that is at the distal end of the device on the tissue to be measured.

7. The handheld tissue oximetry device of claim 1 wherein the at least four wavelengths are approximately 760 nanometers, 810 nanometers, 850 nanometers, and 900 nanometers.

8. The handheld tissue oximetry device of claim 1 wherein at least two of the wavelengths are on either side of the isosbestic point.

9. The handheld tissue oximetry device of claim 1 wherein one of the at least two wavelengths is approximately at the isosbestic point.

10. The handheld tissue oximetry device of claim 1 wherein the processor is adapted to determine the absolute oxygen saturation for the tissue using the concentration values of oxygenated hemoglobin and deoxygenated hemoglobin and not using the concentration values of water and melanin.

11. A handheld tissue oximetry device comprising:

a housing comprising:

a processor contained within the housing;

a memory, contained within the housing, wherein the memory is coupled to the processor;

a display, coupled to the processor, wherein the display is visible from an exterior of the housing;

a battery, contained within the housing, coupled to and supplies power to the processor, memory, and display; and

a tip portion of the housing;

a sensor module, coupled to the processor, wherein the sensor module comprises a probe face that is retained by the tip portion of the housing at a relatively fixed position with respect to the housing and that is placed against and faces tissue to be measured, and the sensor module comprises:

a first plurality of detector structures, formed on the probe face, arranged in a circular arrangement and asymmetrically about a point on a line intersecting a circle of the circular arrangement at a first point and a second point;

a second plurality of detector structures, formed on the probe face, arranged in the circular arrangement and asymmetrically about the point on the line in the circular arrangement;

a first source structure of the sensor module, formed on the probe face, positioned at the first point of the circle of the circular arrangement;

a second source structure of the sensor module, formed on the probe face, positioned at the second point of the circle of the circular arrangement, wherein the first and second source structures emit radiation having at least four wavelengths that are longer than wavelengths of primary absorption peaks of methylene blue;

a first detector structure, formed on the probe face, on the circle of the first plurality of detector structures, wherein a first distance is from the first detector structure to the first source structure, a second distance is

from the first detector structure to the second source structure, and the first distance is greater than the second distance;

a second detector structure, formed on the probe face, on the circle of the first plurality of detector structures, arranged, wherein a third distance is from the second detector structure to the first source structure, a fourth distance is from the second detector structure to the second source structure, and the fourth distance is greater than the third distance;

a third detector structure, formed on the probe face, on the circle of the second plurality of detector structures, wherein a fifth distance is from the third detector structure to the first source structure, a sixth distance is from the third detector structure to the second source structure, the fifth distance is different from the first distance and the second distance, and the sixth distance is different from the first distance and the second distance; and

a fourth detector structure, formed on the probe face, on the circle of the second plurality of detector structures, wherein a seventh distance is from the fourth detector structure to the first source structure, an eighth distance is from the fourth detector structure to the second source structure,

the first distance is different from the second, third, and fourth distances,

the second distance is different from the third and fourth distances,

the third and fourth distances are different, and

the first distance is greater than the second, third, fifth, sixth, seventh, and eighth distances, and the second distance is less than the fifth, sixth, seventh, and eighth distances, and

wherein the processor is adapted to

control the first and second source structures to emit the radiation at the four wavelengths into tissue to be measured,

receive digital reflectance data for detected radiation detected by the first and second plurality of detector structures from the tissue,

calculate a plurality of absorption coefficients using the digital reflectance data for the radiation,

solve a set of reflection coefficient equations using the plurality of absorption coefficients to determine concentration values of oxygenated hemoglobin, deoxygenated hemoglobin, water, and melanin for the tissue, wherein the concentration values of oxygenated hemoglobin and deoxygenated hemoglobin are relatively independent of the concentration values of water and melanin for the tissue,

determine the absolute oxygen saturation for the tissue using the concentration values of oxygenated and deoxygenated hemoglobin, and output from the display a value indicative of the absolute oxygen saturation for the tissue.

12. The handheld tissue oximetry device of claim 11 wherein the at least four wavelengths of radiation are longer than wavelengths of primary absorption peaks of povidone-iodine.

13. The handheld tissue oximetry device of claim 11 wherein at least two of the four wavelengths are approximately 760 nanometers and 850 nanometers.

14. The handheld tissue oximetry device of claim 10 wherein a ninth distance is from the first source structure to

13

the second source structure, and the ninth distance is greater than the first, second, third, fourth, fifth, sixth, seventh, and eighth distances.

15. The handheld tissue oximetry device of claim 11 wherein the first and second source structures emit at least three wavelengths of radiation longer than 730 nanometers.

16. The handheld tissue oximetry device of claim 15 wherein at least three of the wavelengths are approximately 760 nanometers, 810 nanometers, and 850 nanometers.

17. The handheld tissue oximetry device of claim 11 wherein the first source structure is adapted to emit each of the four wavelengths of radiation and the second source structure is adapted to emit each of the four wavelengths of radiation.

18. The handheld tissue oximetry device of claim 11 wherein the at least four wavelengths are approximately 760 nanometers, 810 nanometers, 850 nanometers, and 900 nanometers.

19. The handheld tissue oximetry device of claim 11 wherein at least two of the four wavelengths are on either side of the isosbestic point.

20. The handheld tissue oximetry device of claim 11 wherein one of the four wavelengths is approximately at the isosbestic point.

21. The handheld tissue oximetry device of claim 11 wherein the handheld tissue oximetry device is a standalone unit,

when the handheld tissue oximetry device is used, the housing comprising the processor, memory, display, and battery of the device is cradled between a thumb and forefinger of a hand of a user while the display is at a proximal end of the device and the tip portion of the housing extends in a distal direction to a distal end of the device, and

while the device is in the user's hand, the user positions the probe face that is at the distal end of the device on the tissue to be measured.

22. The handheld tissue oximetry device of claim 11 wherein the housing is a handheld housing.

23. The handheld tissue oximetry device of claim 11 wherein the processor is adapted to determine the absolute oxygen saturation for the tissue using the concentration values of oxygenated hemoglobin and deoxygenated hemoglobin and not using the concentration values of water and melanin.

24. A handheld tissue oximetry device comprising:

a housing comprising:

a processor contained within the housing;

a memory, contained within the housing, wherein the memory is coupled to the processor;

a display, coupled to the processor, wherein the display is visible from an exterior of the housing;

a battery, contained within the housing, coupled to and supplies power to the processor, memory, and display; and

a tip portion of the housing;

a sensor module, coupled to the processor, wherein the sensor module comprises a probe face that is retained by the tip portion of the housing at a relatively fixed position with respect to the housing and that is placed against and faces tissue to be measured, and the sensor module comprises:

a first source structure and a second source structure, each formed on the probe face;

a first source diode and a second source diode, each coupled to the processor and adapted to emit radiation at four wavelengths longer than 730 nanometers;

14

a first radiation directing element and a second radiation directing element, optically coupled, respectively, to the first and second source diodes;

a first optical fiber optically coupled between the first radiation directing element and the first source structure;

a second optical fiber optically coupled between the second radiation directing element and the second source structure, wherein the first waveguide transmits radiation emitted by the first source structure and passed through the first radiation directing element to the first source structure, and the second waveguide transmits radiation emitted by the second source structure and passed through the second radiation directing element to the second source structure;

a first detector structure, formed on the probe face, wherein a first distance is from the first detector structure to the first source structure, a second distance is from the first detector structure to the second source structure, and the first distance is greater than the second distance;

a second detector structure, formed on the probe face, wherein a third distance is from the second detector structure to the first source structure, a fourth distance is from the second detector structure to the second source structure, and the fourth distance is greater than the third distance;

a third detector structure, formed on the probe face, wherein a fifth distance is from the third detector structure to the first source structure, a sixth distance is from the third detector structure to the second source structure, the fifth distance is different from the first distance and the second distance, and the sixth distance is different from the first distance and the second distance; and

a fourth detector structure, formed on the probe face, wherein the first, second, third, and fourth detector structures are arranged asymmetrically about a point on a line on which the first and second source structures are arranged, a seventh distance is from the fourth detector structure to the first source structure, an eighth distance is from the fourth detector structure to the second source structure, the seventh distance is different from the first, second, fifth, and sixth distances, and the eighth distance is different from the first, second, fifth, and sixth distances,

the first distance is greater than the second, third, fourth, fifth, sixth, seventh, and eighth distances, and the second distance is less than the third, fourth, fifth, sixth, seventh, and eighth distances, and

wherein the processor is adapted to:

control the first and second source diodes to emit the radiation at the at least four wavelengths into tissue via the first source structure and a second source structure,

control the first, second, third, and fourth detector structures to detect the radiation at the four wavelengths subsequent to reflection of the radiation from the tissue, receive digital reflectance data for the detected radiation for the four wavelengths collected from the tissue by the first, second, third, and fourth detector structures, calculate a plurality of absorption coefficients using the digital reflectance data;

solve a set of reflection coefficient equations using the plurality of absorption coefficients to determine concentration values of oxygenated hemoglobin, deoxygenated hemoglobin, water, and melanin in the tissue, wherein the concentration values of oxygenated and deoxygen-

15

ated hemoglobin are relatively independent of the concentration values of water and melanin for the tissue, determine the absolute oxygen saturation for the tissue using the concentration values of oxygenated hemoglobin and deoxygenated hemoglobin, and output from the display a value indicative of the absolute oxygen saturation for the tissue.

25. The handheld tissue oximetry device of claim 24 wherein at least two of the four wavelengths are on opposite sides of the isosbestic point for hemoglobin.

26. The handheld tissue oximetry device of claim 24 wherein one of the four wavelengths is substantially at the isosbestic point for hemoglobin.

27. The handheld tissue oximetry device of claim 24 wherein the handheld tissue oximetry device is a standalone unit,

when the handheld tissue oximetry device is used, the housing comprising the processor, memory, display, and battery of the device is cradled between a thumb and forefinger of a hand of a user while the display is at a proximal end of the device and the tip portion of the housing extends in a distal direction to a distal end of the device, and

while the device is in the user's hand, the user positions the probe face that is at the distal end of the device on the tissue to be measured.

16

28. The handheld tissue oximetry device of claim 24 wherein the housing is a handheld housing.

29. The handheld tissue oximetry device of claim 24 wherein the sensor module comprises a first photodetector and a first waveguide, coupled between the first detector structure and the first photodetector.

30. The handheld tissue oximetry device of claim 29 wherein the sensor module comprises an aperture plate, and the aperture plate comprises the first waveguide.

31. The handheld tissue oximetry device of claim 29 wherein the first waveguide comprises a third optical fiber, coupled between the first detector structure and the first photodetector.

32. The handheld tissue oximetry device of claim 24 wherein a ninth distance is from the first source structure to the second source structure, and the ninth distance is greater than the first, second, third, fourth, fifth, sixth, seventh, and eighth distances.

33. The handheld tissue oximetry device of claim 24 wherein the processor is adapted to determine the absolute oxygen saturation for the tissue using the concentration values of oxygenated hemoglobin and deoxygenated hemoglobin and not using the concentration values of water and melanin.

* * * * *

专利名称(译)	光波长选择，以避免手术染料		
公开(公告)号	US9216000	公开(公告)日	2015-12-22
申请号	US13/887178	申请日	2013-05-03
[标]申请(专利权)人(译)	维奥普蒂克斯公司		
当前申请(专利权)人(译)	VIOPTIX INC.		
[标]发明人	BECHTEL KATE LEEANN LLOYD LESTER JOHN		
发明人	BECHTEL, KATE LEEANN LLOYD, LESTER JOHN		
IPC分类号	A61B5/1455 A61B5/00 A61B5/1495 A61B19/00 A61M35/00		
CPC分类号	A61B5/74 A61B5/0075 A61B5/1455 A61B5/1495 A61B5/14551 A61M35/003 A61B5/7282 A61B5/742 A61B5/7405 A61B5/7475 A61B19/54 A61B5/14552 A61B2560/0431 A61B5/0059 A61B5/14546 A61B5 /1459 A61B5/72 A61B5/7246 A61B90/11 A61B90/39 A61B2090/065 A61B2090/306 A61B2090/395 A61B2560/0475 A61B2562/0271 A61B2562/166		
优先权	61/642399 2012-05-03 US 61/642395 2012-05-03 US 61/642393 2012-05-03 US 61/642389 2012-05-03 US 61/682146 2012-08-10 US		
其他公开文献	US20140155716A1		
外部链接	Espacenet USPTO		

摘要(译)

组织血氧测定装置利用至少三种或至少四种不同波长的光来收集反射率数据，其中不同波长长的于730纳米。利用三个或四个波长产生一系列适合于精确测定氧合血红蛋白和脱氧血红蛋白浓度的反射数据。相对长的波长降低了来自某些染料的光学干扰，特别是亚甲蓝和PVPI，其可能存在于被分析组织的生存力上并进一步增强精确反射率数据的产生。波长为760纳米，810纳米和850纳米，或760纳米，810纳米，850纳米和900纳米。

