



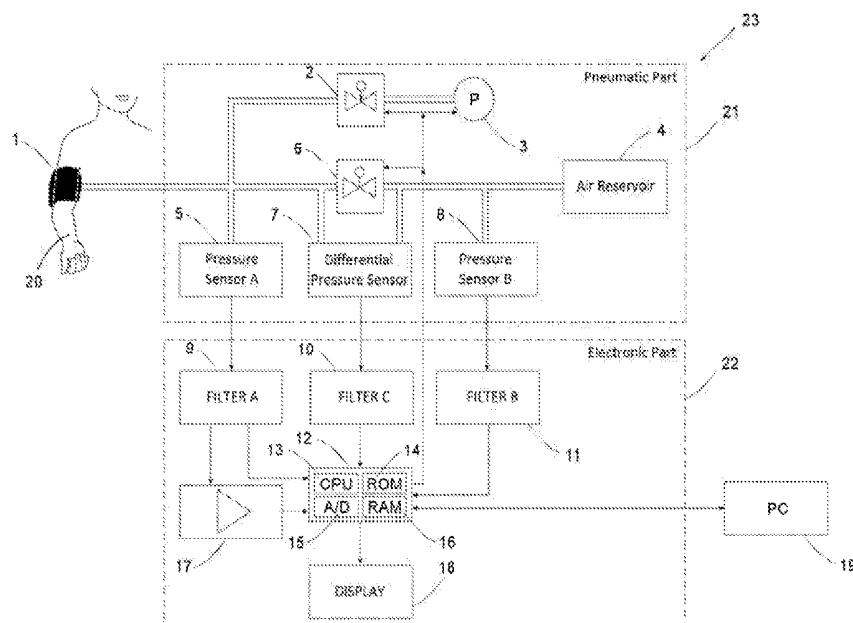
US 20170196468A1

(19) **United States**(12) **Patent Application Publication**  
**FABIAN et al.**(10) **Pub. No.: US 2017/0196468 A1**(43) **Pub. Date: Jul. 13, 2017**(54) **METHOD FOR AN ACCURATE  
AUTOMATED NON-INVASIVE  
MEASUREMENT OF BLOOD PRESSURE  
WAVEFORM AND APPARATUS TO CARRY  
OUT THE SAME***A61B 5/00* (2006.01)*A61B 5/022* (2006.01)(52) **U.S. CL.**CPC ..... *A61B 5/02108* (2013.01); *A61B 5/02233*  
(2013.01); *A61B 5/0235* (2013.01); *A61B*  
*5/6824* (2013.01); *A61B 5/7203* (2013.01)(71) Applicants: **CZECH TECHNICAL UNIVERSITY  
IN PRAGUE, FACULTY OF  
ELECTRICAL ENGINEERING,  
Praha (CZ); CZECH TECHNICAL  
UNIVERSITY IN PRAGUE, CZECH  
INSTITUTE OF INFORMATICS,  
ROBOTICS, Praha (CZ)**(72) Inventors: **Vratislav FABIAN, Praha (CZ); Vaclav  
KREMEN, Praha (CZ); Martin  
DOBIAS, Ricany (CZ)**(73) Assignees: **CZECH TECHNICAL UNIVERSITY  
IN PRAGUE, FACULTY OF  
ELECTRICAL ENGINEERING, Praha  
(CZ); CZECH TECHNICAL  
UNIVERSITY IN PRAGUE, CZECH  
INSTITUTE OF INFORMATICS,  
ROBOTICS, Praha (CZ)**(21) Appl. No.: **15/401,338**(22) Filed: **Jan. 9, 2017**(30) **Foreign Application Priority Data**

Jan. 7, 2016 (CZ) ..... PV 2016-6

**Publication Classification**(51) **Int. Cl.***A61B 5/021* (2006.01)*A61B 5/0235* (2006.01)(57) **ABSTRACT**

An apparatus for an accurate automated non-invasive measurement of blood pressure waveform using brachial (occlusion) cuff pressurized above systolic pressure and using differential pressure sensor. The methodology involves measurement in suprasystolic mode and in utilization and construction of the device followed by algorithms for processing and analysis of measured blood pressure pulse waves and assessment of hemodynamic parameters of human cardiovascular system. The device includes an electro-pump connected to the collar device, a differential pressure sensor, pressure sensor A, pressure sensor B, valve, closing a valve and the air reservoir. The cuff is wrapped around a person's arm. The values of the instantaneous pressure in the pneumatic portion of the device are converted into an electric signal by the pressure sensor A, pressure sensor B and the differential pressure sensor. These signals are then filtered using a set of passive RC elements for filtering out high frequency interference, and fed to the microprocessor with a computing unit, analog to digital converter. The sampling frequency is sensed signal at least 200 Hz. The control algorithm in the microprocessor, according to signals from the pressure sensor A further controls the course of cuff pressurization, controls the control valve, and finally determines the closing and opening of the closing valve. A microprocessor further controls a display and the data may be transmitted to the PC.



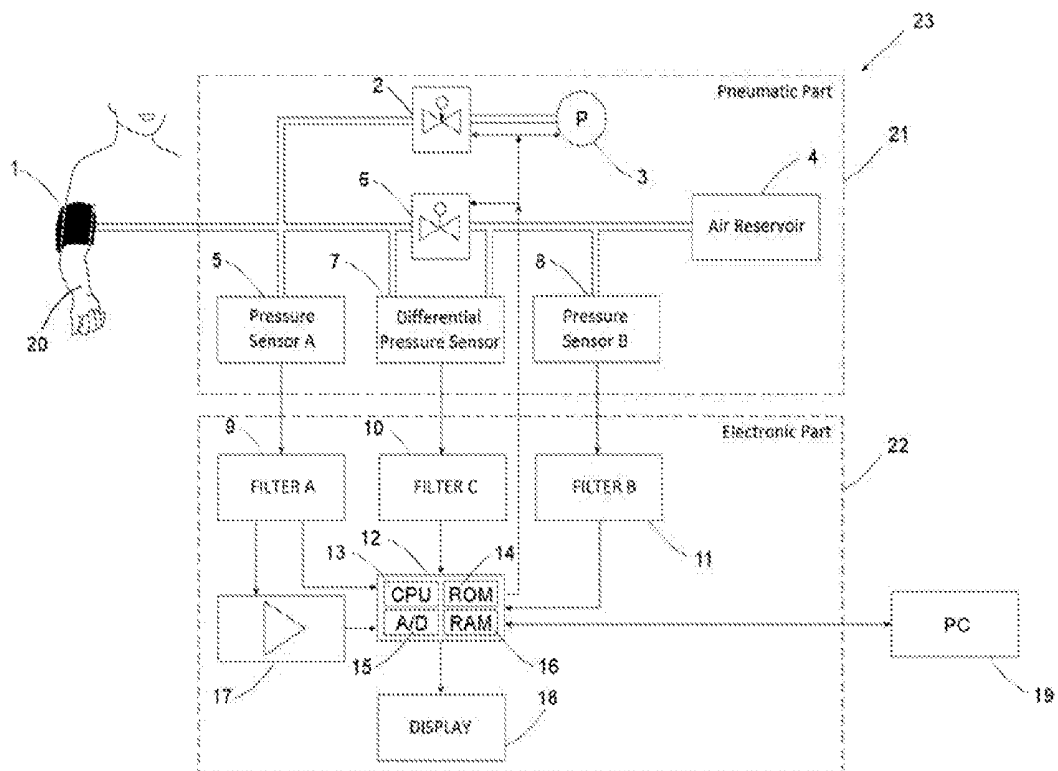


FIG. 1

**METHOD FOR AN ACCURATE  
AUTOMATED NON-INVASIVE  
MEASUREMENT OF BLOOD PRESSURE  
WAVEFORM AND APPARATUS TO CARRY  
OUT THE SAME**

**BACKGROUND AND SUMMARY**

**[0001]** The present application claims priority to Czech Republic Patent Application PV 2016-6, filed Jan. 7, 2016, which is incorporated by reference. The technical solution concerns a method for accurate automated non-invasive measurement of blood pressure waveform and the apparatus to carry out the method. By using the device and the method, and based on measured signals processed by developed algorithms it is possible to effectively determine important hemodynamic parameters of cardiovascular system. This device is intended for use in human and veterinary medicine, especially in the investigation of the state of cardiovascular system, i.e. hemodynamic parameters of bloodstream.

**[0002]** Devices for determination of hemodynamic parameters of cardiovascular system based on measurement of pressure waves are widely used in human medicine. They enable to determine many advanced hemodynamic parameters that enable complex assessment of cardiovascular system including pulse wave velocity (PWV), augmentation index (AIx) that serves as basic parameters for assessment of Arterial Stiffness (AS) and risk of development and progression of arteriosclerosis and associated comorbidities.

**[0003]** Superior and most precise method for assessment of above-mentioned parameters still remains invasive measurement by catheter introduced to aortic root. This is still invasive operating procedure associated with certain known health risks and high price. The examination can't be performed under ambulatory conditions and have to be performed by certified interventional cardiologist in specially equipped operating room for angiology including catheter and other equipment to perform this type of surgery.

**[0004]** Non-invasive substitution of the invasive method is described in patent U.S. Pat. No. 6,117,087 and uses contact pressure sensor and sophisticated mathematical models derived from limited amount of data measured of patients with indications of several cardiovascular diseases. Learning models under such circumstances introduces high infidelity into the method.

**[0005]** Another solution is described in Czech patent number 295119, where measurement of blood pressure pulse wave is accomplished by contact pressure sensor connected to differential pressure sensor that increases sensitivity of measured pressure curve. This solution enables to measure very small blood pressure pulse waves from the surface of pressurized arteries at radial arteries with option of PWV analysis using special setup of device and utilization of two sensors, while there is no constriction of measured artery by the device. Placement of the device at radial artery is main limitation of the method to assess central aortic pulse wave as well as brachial pulse wave. This is because of known physiological phenomenon that describes change of pattern and amplitude of pulse wave in a particular place if measured from the aortic root distally along arm compare to pulse wave measured in the aortic root. This phenomenon applied to the method suggests that the method has substantial inaccuracy as well.

**[0006]** Main disadvantages of devices that use contact pressure sensor (e.g. Sphygmocor CVMS by AtCor) are

changes of sensed pulse wave that are introduced by movements of examiner (physician) and by patient during measurement. These changes generate inaccuracies. Another main disadvantage of the method is that measurement can't be carried out automatically and it needs trained medical personnel.

**[0007]** SphygmoCor XCEL (AtCor), Arteriograph (ColsonMed) BP+ (Colson) that determine hemodynamic parameters of cardiovascular system from pattern of suprasystolic pressure pulse waves doesn't offer solution of above-mentioned disadvantages. Measurement is carried out automatically and by using arm cuff for measurement of suprasystolic pressure pulse waves. As described in patent WO 2005077265 A1, these pulsations are sensed using suprasystolic pressure (preferred is a systolic pressure +35 mmHg) by standard pressure sensor used in devices for blood pressure measurement by standard oscilometric principle. Typical dynamic range of these sensors is usually min 40 kPa, and relative overpressure ~300 mmHg. Because of small amplitudes of suprasystolic pressure pulse waves device in patent WO 2005077265 A1 uses compensation filter ("reverse filter") that a circuit that compensates for pattern of the signal during measurement. This method is burdened by inaccuracy and under discussion in scientific press—e.g. discussed in Validation of the Arteriograph working principle: questions still remain. Bram Trachet et al. Journal of Hypertension, 29:619-622, 2011. This remains similar also for patents US 2014135632 A1 and US 2010256507A1. Another disadvantage of above-mentioned devices is a complexity of mathematical models for assessment of hemodynamic parameters. These models are derived from limited set of the data and highly multivariate. They also need certain high amount of input parameters they use together with measured pressure pulse wave to be able to calculate a result. Other several sensors often supply these input parameters. Used models were often tested using limited sizes of study populations and limited types of cardiovascular diseases, which can introduce certain instabilities and inaccuracies into models and thus into the whole measurement system.

**[0008]** In an aspect of the present invention, accurate automated non-invasive measurement of blood pressure waveform according to the invention is provided. Its essence consists in the following method of measurement and in the following apparatus embodiment. The device consists of an electromechanical pump connected to an arm cuff, a differential pressure sensor, a pressure sensor A, a pressure sensor B, a control (decompression) valve, a closing valve and an air reservoir, with a minimal volume of 50 ml. Arm cuff is wrapped around the arm of the examined person and just tightened. Actual values of the pressures in the pneumatic components of the apparatus are converted into an electrical signal by the pressure sensor A, the pressure sensor B and the differential pressure sensor. These signals are then filtered using a set of passive RC low pass filters to remove high frequency interference, and thereafter through analog to digital converter (at least 12-bit) they are digitized and ready for further computer processing. The signal from pressure Sensor A is after filtration amplified by an amplifier, approximately 50 to 100 times. The sampling frequency of the signal is at least 200 Hz. The control element, based on the current sensed values from the pressure sensor A and by casing the electromechanical pump, and the control and closing valves, controls and monitors the course of the cuff

inflation during measurement. The control element (e.g. a microprocessor) senses, processes and evaluates the measured data that can be displayed directly on the display, or may be transferred to a PC for further processing.

**[0009]** In the first phase of measurement, the apparatus device according to the invention begins to inflate the arm cuff bladder via electromechanical pump, at a rate controlled by the control element, e.g. a microprocessor. The cuff inflation speed is gradually slowed down so that the pneumatic system reaches a specified value of suprasystolic pressure. Through the closing valve, which is located between the inputs of the differential pressure sensor, and which is at this phase of measurement in open position, is inflated the air reservoir, which serves to minimize pressure variations in the pneumatic system. During the controlled inflation of the pneumatic system, the processor continually evaluates oscillometric pulsations obtained by digitalization of filtered and amplified signal from the pressure sensor A. Based on measured oscillometric pulsations during cuff inflation and cuff pressure signal from unamplified pressure sensor A, the value of suprasystolic pressure is determined by the control element (e.g. a microprocessor). The value of suprasystolic pressure is at least 30 mmHg higher than a systolic pressure of measured person. Pneumatic system is inflated to the suprasystolic pressure by an electromechanical pump before starting the measurement of blood pressure waveform.

**[0010]** A necessary condition for quality measurement of the pulse pressure wave by the apparatus according to the invention is to achieve suprasystolic pressure in the cuff placed on the arm over the brachial artery. After reaching the suprasystolic pressure and its stabilization, i.e. the pressure drop in the pressure sensors A and B is less than 1 mmHg/min, there is a signal from the processor to trigger the closing valve, i.e. the valve is closed. This separates the inputs of differential pressure sensor, i.e. separation of the static cuff pressure from pressure with superimposed pressure pulsations. At output of the differential sensor with a range of hundreds of Pa—preferred  $\pm 250$  Pa or  $\pm 500$  Pa, i.e. approx.  $\pm 1.88$  mmHg, respectively  $\pm 3.75$  mmHg, appears blood pulse wave signals—pressure pulsations, separated from the static pressure cuff. Next phase of measurement is suprasystolic pressure pulsations measurement. During this phase, the tightness in separate parts of a pneumatic system is monitored using the signals from the pressure sensors A and B. This procedure yields a signal that is up to 100 times more sensitive compare to existing methods of suprasystolic pressure pulsations measurement. This thus eliminates disadvantages of existing devices for the automatic measurement suprasystolic pressure pulsations, in particular the need of using a compensation filter or derived complex multivariate models.

**[0011]** After suprasystolic pressure pulsations measurement is finished, a control element (e.g. a microprocessor) opens the closing valve and by regulation (decompression) valve gradually releases the cuff pressure, and pressure throughout the whole pneumatic system. During the controlled deflation the oscillometric pulsations from pressure sensor A are measurement and therefore it is possible to measure blood pressure—systolic, diastolic, mean arterial, using standard oscillometric method.

**[0012]** System automatically determines actual heart rate of the person using analysis of measured data. Other hemodynamic parameters of cardiovascular system of examined

person are automatically determined from the pattern of the signal, e.g. systolic and diastolic blood pressure of each heartbeat, pulse wave velocity (PWV), augmentation index (AIx), central aortic pressure, area under the curve and the maximum pressure amplitude, which reflects the instantaneous stroke volume, and others.

**[0013]** The measured pressure curve is accurate and corresponds to the brachial pulse wave otherwise invasively measured by a catheter placed in patient's arm. The apparatus according to the invention is accurate, portable, and inexpensive and is usable even in individuals with cardiovascular disease, or cardiovascular system status changes. To operate the device is simple and it is easy to learn. Patient themselves are able to perform the measurement after a short learning practice period. It allows carrying out measurements in outpatient settings, such as surgery cardiologists, internists and general practitioners, but also at home environment. The whole one trial of scanning procedure takes at maximum mo minutes and it does not burden or harm the patient.

#### BRIEF DESCRIPTION OF THE DRAWINGS

**[0014]** The invention is illustrated using the attached drawing, wherein FIG. 1 is a block diagram of an exemplary apparatus according to the invention.

#### DETAILED DESCRIPTION

**[0015]** There is a block diagram of device **23** according to the invention in the FIG. 1. The device for non-invasive measurement of suprasystolic pressure pulsations of the invention implemented by a microprocessor **12** with a 24-bit A/D converter **15** with a sampling frequency of 200 Hz. Inflating the pneumatic part **21** of the device **23**, including the occlusive cuff **1**, which is located in the patient arm **20** and the air reservoir **4** of 100 ml volume, is carried out by electromechanical pump **3**. Control (decompression) valve **2** is located between the inputs of the differential pressure sensor **7** and is controlled, as well as the process of inflating the pneumatic part **21**, by computing unit **13** of the microprocessor **12**, according to an algorithm stored in the program memory of the microprocessor (ROM) **14**. Signals measured from the pressure sensor A **5**, pressure sensor B **8** and the differential pressure sensor **7** are preprocessed using a filter A **9**, filter B **10** and filter C **11**—RC low pass filters to eliminate high frequency interference, and an amplifier of oscillometric pulsations **17** and are stored in the data memory (RAM) **16** of the microprocessor **12**. Digitalized data can be transmitted to the PC **19** for additional processing and simultaneously displayed on the display **18**. Electronic part **22** of the device **23**, the differential pressure sensor **7**, the pressure sensor A **5**, pressure sensor B **8**, the electromechanical pump **3**, the control (decompression) valve **2** and the closing valve **6** are powered by batteries.

**[0016]** In the device for an accurate automated non-invasive measurement of blood pressure waveform using brachial (occlusion) cuff pressurized above systolic pressure and using differential pressure sensor. Methodology involves measurement in suprasystolic mode and in utilization and construction of the device followed by algorithms for processing and analysis of measured blood pressure pulse waves and assessment of hemodynamic parameters of human cardiovascular system. The device comprises an electro-pump (**4**) connected to the collar device (**1**), the

differential pressure sensor (7), pressure sensor A (6), pressure sensor B (8), valve (2), closing a valve (6) and the air reservoir (4). Cuff (1) is wrapped around the arm persons under investigation (20). The values of the instantaneous pressure in the pneumatic portion (21) of the device (23) are converted into an electric signal by the pressure sensor A (6), pressure sensor B (8) and the differential pressure sensor (7). These signals are then filtered using a set of passive RC elements (9), (10), (11) for filtering out high frequency interference, and fed to the microprocessor (12) with a computing unit (13), analog to digital converter (15). The sampling frequency is sensed signal at least 200 Hz. The control algorithm in the microprocessor (12), according to signals from the pressure sensor A (6) further controls the course of cuff pressurization, controls the control valve (2), and finally determines the closing and opening of the closing valve (6). A microprocessor (12) further controls a display (18) and the data may be transmitted to the PC (19).

[0017] The device according to the invention finds an application in civilian use of individual care for non-invasive monitoring of hemodynamic parameters of the cardiovascular system and for a prognosis of cardiovascular diseases, in the area of medical care and postoperative monitoring of patients, but also in preventive medical care, and thereby preventing cardiovascular disease and its comorbidities.

What is claimed is:

1. A method for accurate automated non-invasive measurement of blood pressure pulse waves, comprising:
  - wrapping an arm cuff around an arm of a person to be examined person;
  - inflating the arm cuff and slowing a speed of cuff inflation so that a value of a suprasystolic pressure at least 30 mmHg higher than the systolic pressure of the person is reached in a pneumatic part comprising the arm cuff, sensing suprasystolic pressure pulsations,

converting sensed suprasystolic pressure pulsations into electrical signals,

filtering the electrical signals to eliminate high frequency interference and provide filtered electrical signals,

digitizing the filtered electrical signals for computer processing.

2. The method according to claim 1, comprising, after inflating the arm cuff, performing a controlled deflation of the arm cuff, and detecting oscillometric pulsation during the controlled deflation for measurements of systolic, diastolic and mean pressure using a standard oscillometric method.

3. A device for performing the method according to claim 1, comprising a pneumatic part comprising the arm cuff and an air reservoir, the arm cuff and the air reservoir being connected with an electromechanical pump, a differential pressure sensor, a first pressure sensor, a second pressure sensor, a control valve, and a closing valve, which are connected to an electronic part comprising a control element comprising computing unit, program memory, data memory, and analog-digital converter.

4. The device according to claim 3, wherein a sampling frequency of signals in the control element is 180 Hz to 220 Hz.

5. The device according to claim 3, wherein the closing valve is controlled by the control element to pneumatically separate, after reaching the suprasystolic pressure, pressure in the air reservoir from pressure superposed suprasystolic blood pressure pulsations in the arm cuff.

6. The device according to claim 3, wherein the first and second pressure sensors are arranged to monitor pressure drop in the pneumatic part during measurement of suprasystolic pressure pulsations.

\* \* \* \* \*

|                |                                                                     |         |            |
|----------------|---------------------------------------------------------------------|---------|------------|
| 专利名称(译)        | 精确自动无创测量血压波形的方法及其实现方法                                               |         |            |
| 公开(公告)号        | <a href="#">US20170196468A1</a>                                     | 公开(公告)日 | 2017-07-13 |
| 申请号            | US15/401338                                                         | 申请日     | 2017-01-09 |
| [标]申请(专利权)人(译) | 捷克TECHN UNIV与布拉格FACULTY电气工程                                         |         |            |
| 申请(专利权)人(译)    | 捷克技术大学在布拉格，师资队伍电气工程                                                 |         |            |
| 当前申请(专利权)人(译)  | 捷克技术大学在布拉格，师资队伍电气工程                                                 |         |            |
| [标]发明人         | FABIAN VRATISLAV<br>KREMEN VACLAV<br>DOBIAS MARTIN                  |         |            |
| 发明人            | FABIAN, VRATISLAV<br>KREMEN, VACLAV<br>DOBIAS, MARTIN               |         |            |
| IPC分类号         | A61B5/021 A61B5/0235 A61B5/00 A61B5/022                             |         |            |
| CPC分类号         | A61B5/02108 A61B5/02233 A61B5/7203 A61B5/6824 A61B5/0235 A61B5/0225 |         |            |
| 优先权            | 20166 2016-01-07 CZ                                                 |         |            |
| 其他公开文献         | US10251567                                                          |         |            |
| 外部链接           | <a href="#">Espacenet</a> <a href="#">USPTO</a>                     |         |            |

#### 摘要(译)

一种用于使用在收缩压以上加压的肱动脉（闭塞）套囊并使用差压传感器进行血压波形的精确自动无创测量的装置。该方法涉及在收缩压模式和装置的利用和构建中的测量，随后是用于处理和分析测量的血压脉搏波和评估人类心血管系统的血液动力学参数的算法。该装置包括连接到套环装置的电动泵，差压传感器，压力传感器A，压力传感器B，阀，关闭阀和储气罐。袖口缠绕在一个人的手臂上。瞬时压力的值通过压力传感器A，压力传感器B和压差传感器将装置的气动部分转换成电信号。然后使用一组无源RC元件对这些信号进行滤波，以滤除高频干扰，并通过计算单元模数转换器将其馈送到微处理器。采样频率是至少200Hz的感测信号。微处理器中的控制算法根据来自压力传感器A的信号进一步控制袖带加压的过程，控制控制阀，最后确定关闭阀的关闭和打开。微处理器还控制显示器，并且数据可以传输到显示器PC。

