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(54) **HEART RATE MONITOR**

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22, 2015.

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A61B 5/024 (2006.01)
A61B 5/00 (2006.01)

(52) **U.S. Cl.**
CPC **A61B 5/02438** (2013.01); **A61B 5/681**
(2013.01); **A61B 5/7207** (2013.01); **A61B**
5/6824 (2013.01); **A61B 5/7275** (2013.01);
A61B 5/7282 (2013.01)

(58) **Field of Classification Search**
CPC A61B 5/7207; A61B 5/11; A61B 5/024
See application file for complete search history.

(56) **References Cited**

U.S. PATENT DOCUMENTS

8,180,591 B2	5/2012	Yuen et al.	
8,920,332 B2	12/2014	Hong et al.	
2003/0120164 A1 *	6/2003	Nielsen	A61B 5/02055 600/513
2007/0051369 A1	3/2007	Choi et al.	

(Continued)

OTHER PUBLICATIONS

Peng et al (Motion artifact removal from photoplethysmographic
signals by combining temporally constrained independent compo-
nent analysis and adaptive filter, 2014, BioMedical Engineering
OnLine, 13(50): pp. 1-14).*

(Continued)

Primary Examiner — Patricia Mallari

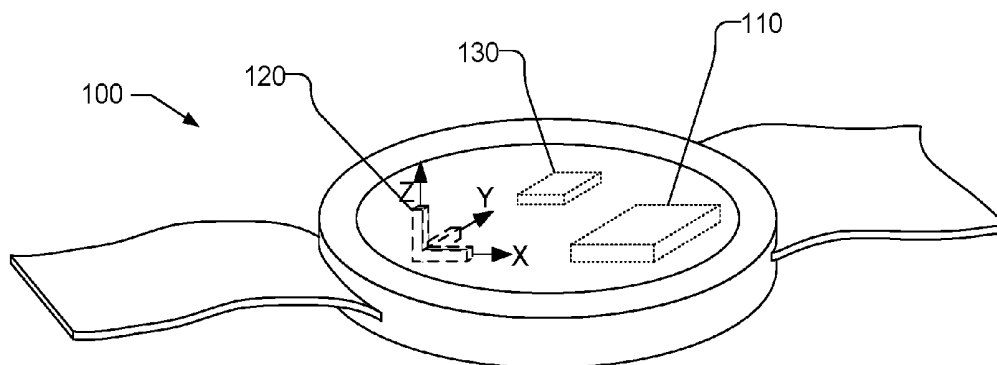
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(57) **ABSTRACT**

A wrist worn heart rate monitor includes a photoplethysmo-
gram (PPG) sensor and an inertial sensor. Signals from the
inertial sensor are used to identify and remove noise from
the PPG signals. An initial heart rate value is selected from
a number of heart rate candidates that remain in the resulting
PPG spectrum and is used to track the heart rate of the user.
The PPG spectrum is monitored while tracking the heart rate
to determine if the selected initial heart rate value is in error.
The PPG spectrum may be monitored by determining a
correlation of possible heart rate candidates in each PPG
spectrum to the previous heart rate candidates and resetting
the heart rate value accordingly. Additionally or alterna-
tively, the PPG spectrum may be monitored by determining
when only a single heart rate candidate is present in con-
secutive PPG spectra and resetting the heart rate value
accordingly.

16 Claims, 6 Drawing Sheets



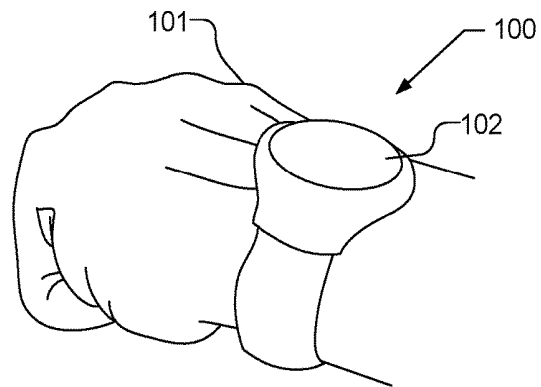


Fig. 1

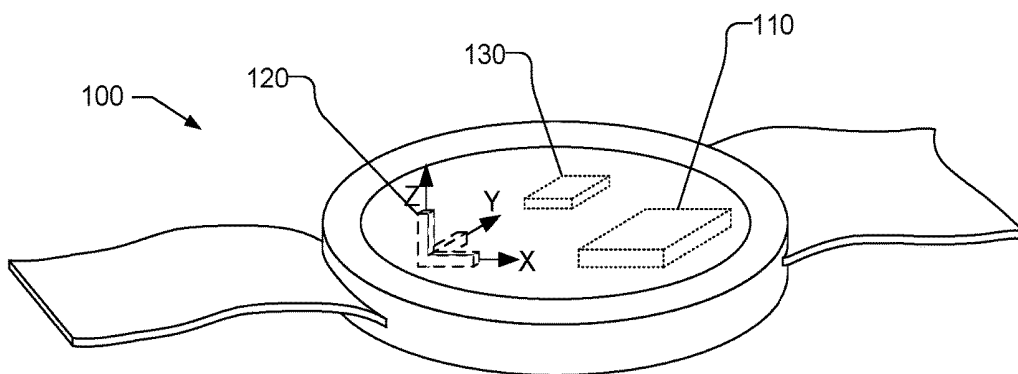


Fig. 2

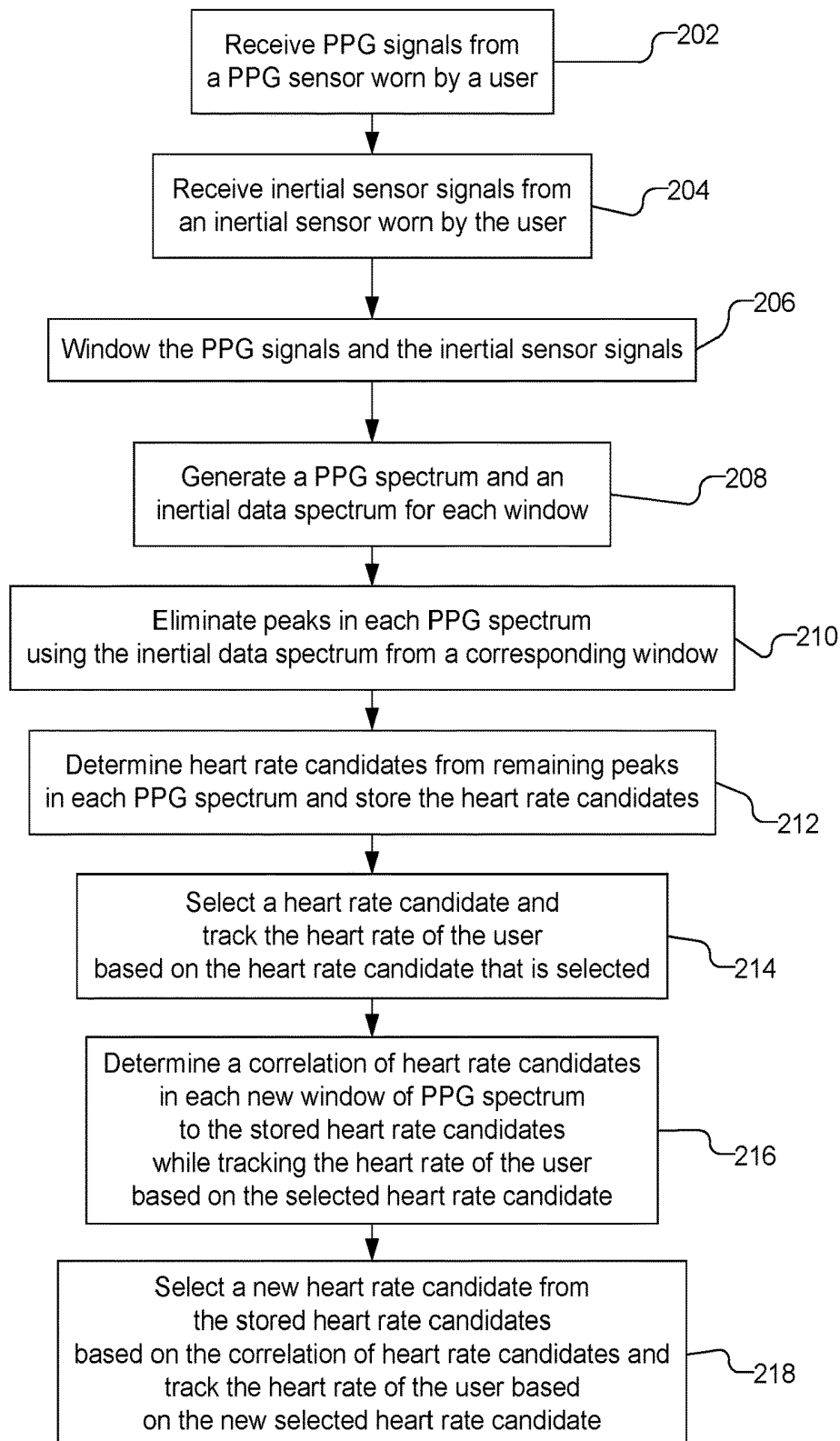


Fig. 3

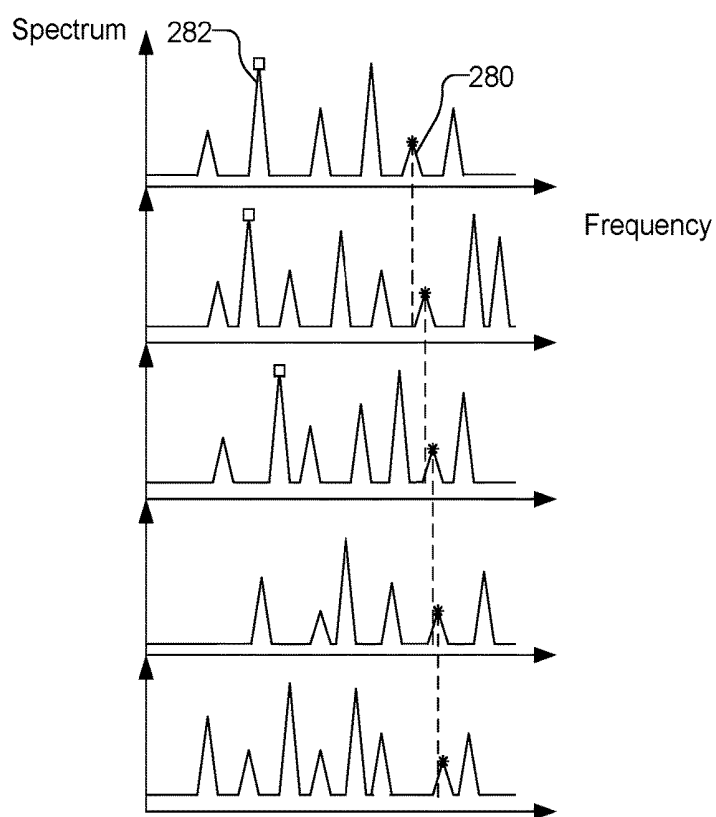


Fig. 4

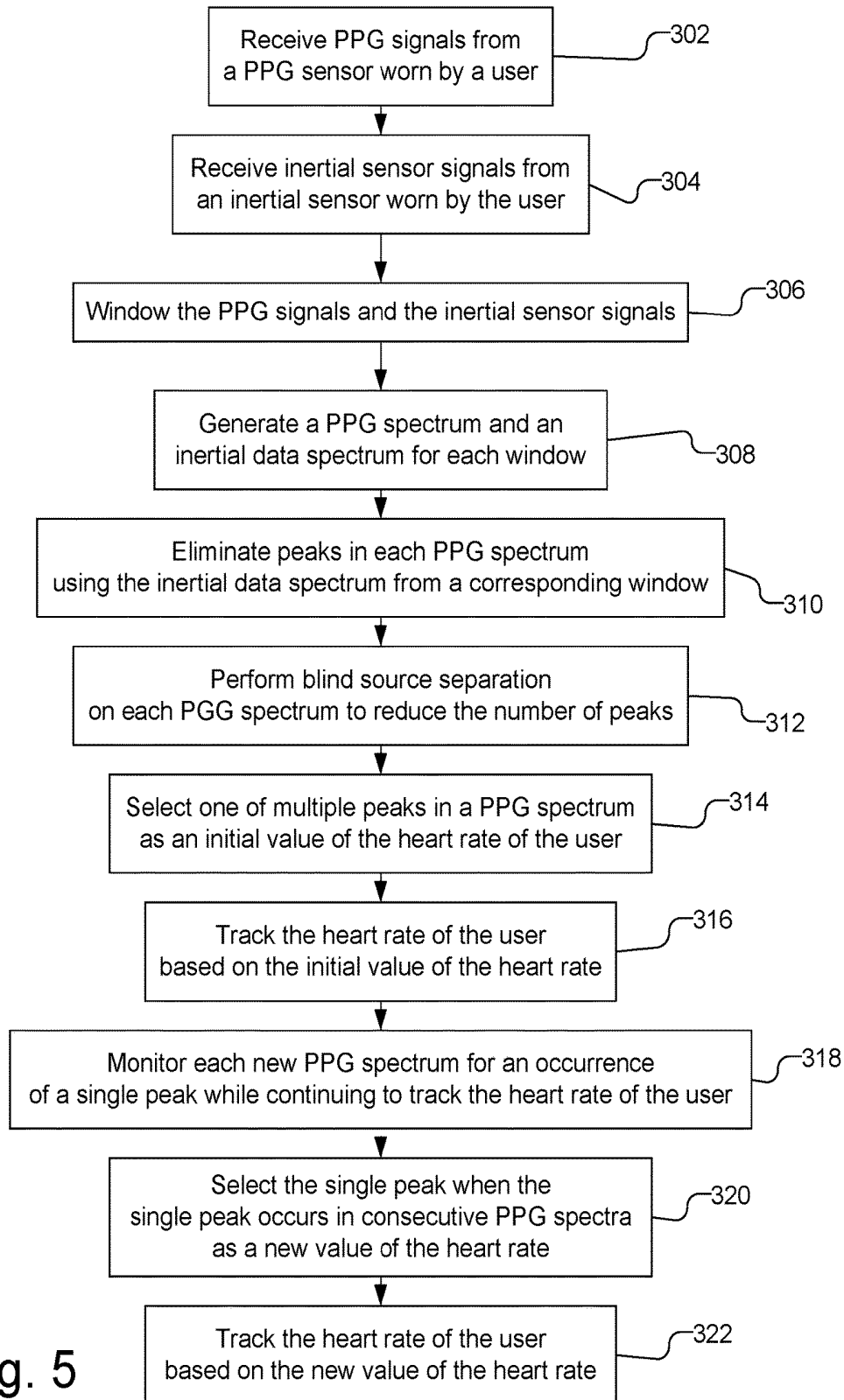
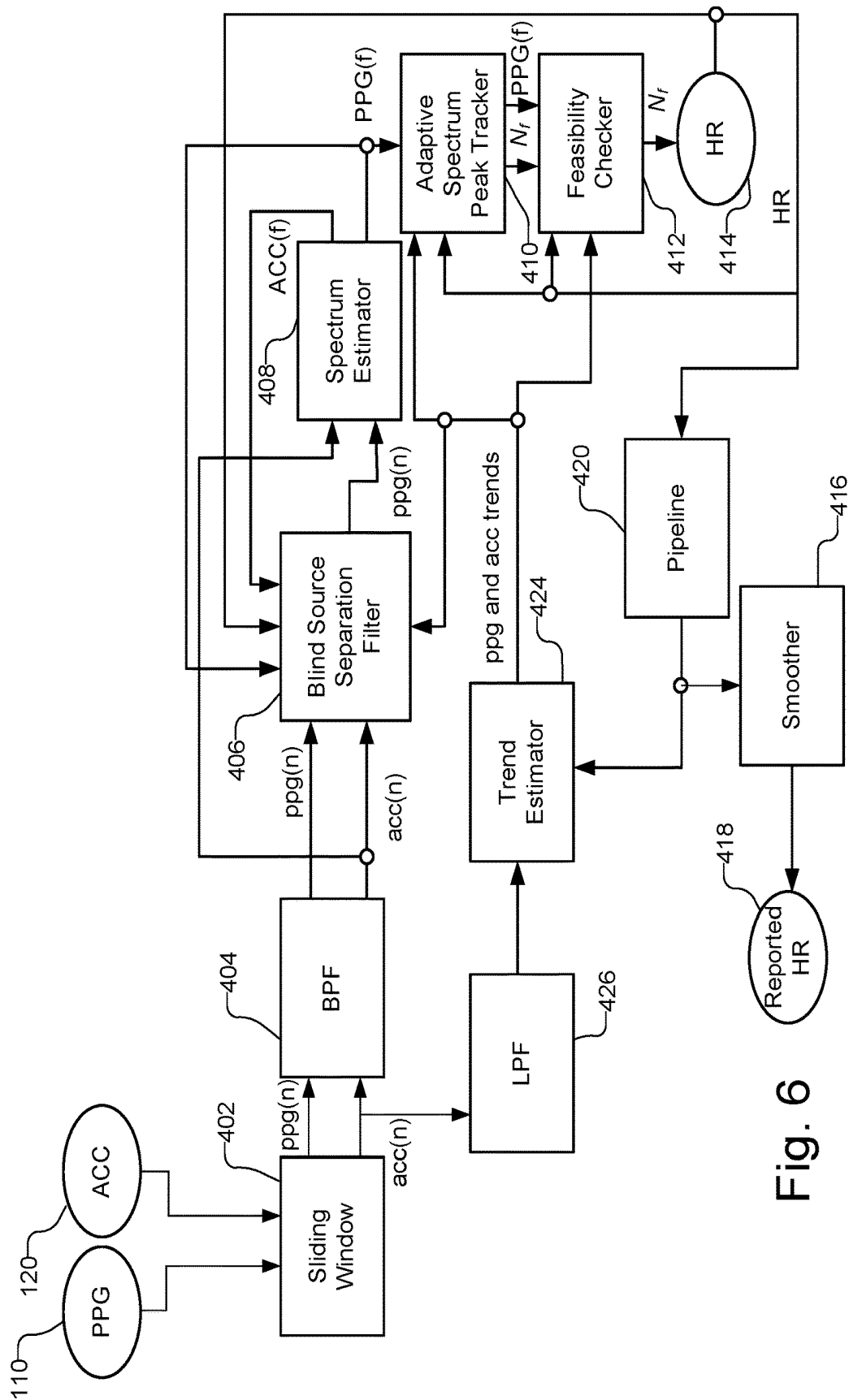


Fig. 5



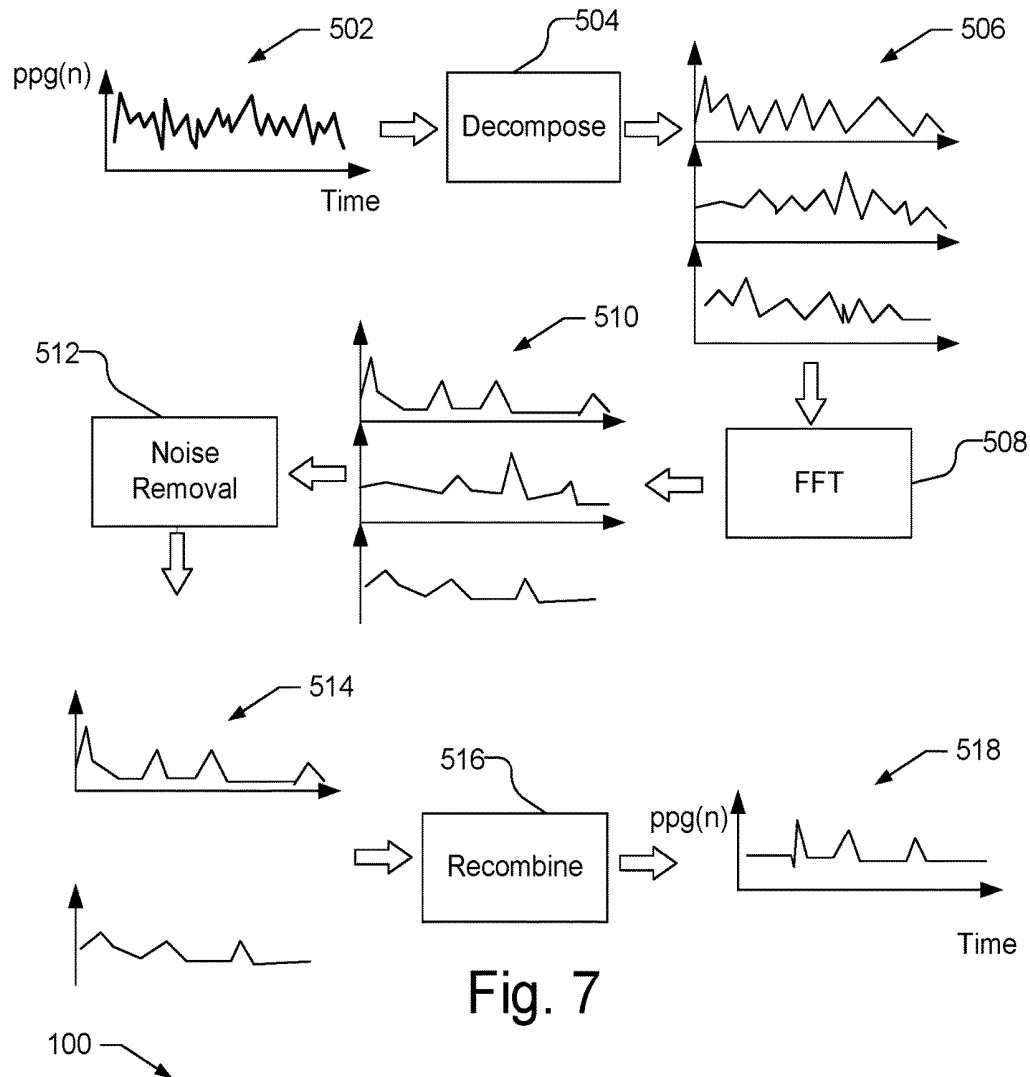


Fig. 7

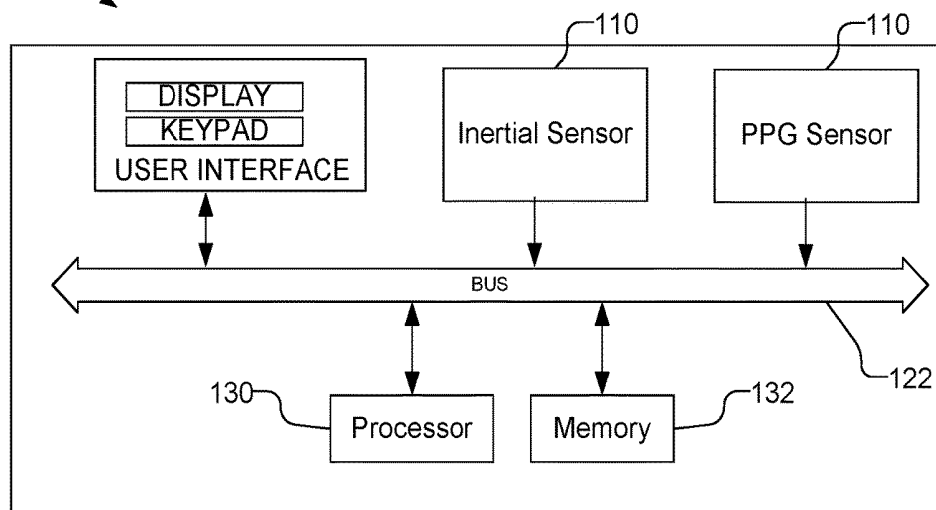


Fig. 8

1

HEART RATE MONITOR**CROSS REFERENCE TO RELATED APPLICATIONS**

This application claims priority under 35 USC 119 to U.S. Provisional Application No. 62/195,730, filed Jul. 22, 2015, which is incorporated by reference herein in its entirety.

FIELD OF THE INVENTION

The present invention relates to a heart rate monitor, and more specifically to a heart rate monitor that is worn on the user's wrist.

BACKGROUND

Heart rate monitors are used for measurement of a heart rate, e.g., for applications such as health monitoring, sports training, and fitness. Conventional devices capable of constantly monitoring a user's heart rate have been, until recently, cumbersome. For example, heart rate monitors often use electrocardiogram (EKG) signals, which require electrodes or a strap placed around the user's chest.

A less cumbersome technique for monitoring heart rate is based on pulse oximetry using a photoplethysmograph (PPG) sensor. A PPG sensor non-invasively measures the absorption of light passing through a user's tissue, e.g., a finger or an ear lobe, to determine the oxygen saturation level of arterial blood and heart rate. Arteries expand and contract due to blood flow and, thus, the amount of absorbed light changes in the course of a heart beat. The resulting signal is referred to as a photoplethysmograph (PPG). The PPG signal may be analyzed to determine, among other thing, the heart rate of the person to which the PPG sensor is attached.

Conventionally, pulse oximetry requires the user to remain relatively motionless to ensure that a good PPG signal is received. When a PPG sensor is used with a person that is in motion, artifacts in the PPG signal may be produced as a result of the user's motion as well as displacement of the PPG sensor. The resulting artifacts or noise result often result in inaccuracies in the estimated heart rate of the user.

SUMMARY

A wrist worn heart rate monitor includes a photoplethysmogram (PPG) sensor and an inertial sensor. Signals from the inertial sensor are used to identify and remove noise from the PPG signals. An initial heart rate value is selected from a number of heart rate candidates that remain in the resulting PPG spectrum and is used to track the heart rate of the user. The PPG spectrum is monitored while tracking the heart rate to determine if the selected initial heart rate value is in error, and if so, the heart rate value is reset. The PPG spectrum may be monitored by determining a correlation of possible heart rate candidates in each PPG spectrum to the previous heart rate candidates and resetting the heart rate value accordingly. Additionally or alternatively, the PPG spectrum may be monitored by determining when only a single heart rate candidate is present in consecutive PPG spectra and resetting the heart rate value accordingly.

BRIEF DESCRIPTION OF THE DRAWINGS

FIG. 1 illustrates a wrist worn heart rate monitor worn on the wrist of a user.

2

FIG. 2 schematically illustrates a wrist worn heart rate monitor.

FIG. 3 is a flow chart illustrating a process of resetting the heart rate monitoring in accordance with one implementation.

FIG. 4 illustrates a number of PPG spectra over five consecutive windows.

FIG. 5 is a flow chart illustrating a process of resetting the heart rate monitoring in accordance with another implementation.

FIG. 6 is an architecture diagram for the heart rate monitor.

FIG. 7 illustrates the operation of a blind source separation filter in the heart rate monitor.

FIG. 8 is a block diagram of the heart rate monitor.

DETAILED DESCRIPTION

FIG. 1 illustrates a wrist worn heart rate monitor **100** worn on the wrist of a user **101** and FIG. 2 schematically illustrates the wrist worn heart rate monitor **100**. Portions of wrist bands are illustrated in FIG. 2 as extending from the sides of the heart rate monitor **100**. The heart rate monitor **100** includes a PPG sensor **110**, a multiple axis inertial sensor **120**, and a processor **130**. The processor **130** is coupled to receive the PPG signals from the PPG sensor **110** and the inertial sensor signals from the inertial sensor **120**. The PPG sensor **110**, the inertial sensor **120**, and processor **130** are inside the heart rate monitor **100** and accordingly are illustrated with dotted lines. The processor **130** monitors the heart rate of the user **101** (shown in FIG. 1) based on the PPG signals and inertial sensor signals. The inertial sensor **120** may be, e.g., a 3 axis accelerometer, where the various axes are labeled X, Y, and Z in FIG. 2. The heart rate monitor **100** may further include a user interface **102** that may display information, such as heart rate, time, etc., to the user, as well as serve as a touch pad for user input. If desired, the heart rate monitor **100** may include hard buttons (not shown) for user input.

The PPG sensor **110** may be a conventional PPG sensor that illuminates the skin of user **101** and measures changes in the absorption of reflected light to monitor the perfusion of blood to the dermis and subcutaneous tissue of the skin. As the heart pumps blood to the user's wrist, the pressure pulse will distend the arteries and arterioles in the subcutaneous tissue. The change in volume caused by the pressure pulse is detected by the PPG sensor **110** by illuminating the skin with light, e.g., from a light-emitting diode (LED) and measuring the amount of light reflected to a photodiode in the PPG sensor **110**.

With the heart rate monitor **100** worn on the wrist of the user **101**, however, motion incurred during normal activity or exercise will produce artifacts, referred to herein as noise, in the PPG signal produced by the PPG sensor **110**. Moreover, the PPG sensor **110** may be displaced with respect to the user's skin during normal activity or exercise, resulting in additional noise in the PPG signal. Additional sources of noise in the PPG signal may also be present, physiological phenomena that happen inside the body and hardware noise.

The processor **130** receives the PPG signals from the PPG sensor **110** and generates a PPG spectra in discrete windows. A PPG spectrum in a window, however, may include multiple peaks, with one peak corresponding to the user's heart rate, while the remaining peaks correspond to noise in the PPG signal. The peak associated with the user's heart rate will typically be a non-dominant peak and is, therefore, difficult to identify. Accordingly, the processor **130** may use

the inertial sensor signals from the inertial sensor **120** to identify and remove noise peaks in the PPG signal. Once the peak corresponding to the user's heart rate is identified, the heart rate is tracked using the identified heart rate as an initial heart rate and adjusting the estimated heart rate based on estimated changes in the heart rate, i.e., whether the heart rate is increasing, decreasing or is constant. Even after removal of noise in the PPG signals, however, the resulting PPG spectrum may still include multiple peaks, only one of which corresponds to the heart rate. If a peak that is associated with noise is incorrectly identified as the initial heart rate, the heart rate will be tracked based on an incorrect initial heart rate, resulting in an inaccurate estimate of the heart rate. Accordingly, the processor **130** includes a reset through which the processor **130** may recognize an error in the selection of the initial heart rate has occurred and may select a new initial value of the user's heart rate.

FIG. 3 is a flow chart illustrating a process of resetting the heart rate monitoring in accordance with one implementation. As illustrated, PPG signals from PPG sensor **110** worn by a user are received (**202**). Additionally, inertial sensor signals from an inertial sensor **120**, which may be accelerometers, worn by the user are received (**204**). The PPG sensor and inertial sensor are worn on the wrist of the user. The PPG signals and the inertial sensor signals are windowed (**206**). In other words, a sliding time window of T seconds, e.g., T=2 seconds, is applied to the PPG signals and the inertial sensor signals. The window may slide so that every S seconds, e.g., $S \leq T$, a new window of PPG signals and the inertial sensor signals is produced. A PPG spectrum and inertial data spectrum are generated for each window of the PPG signals and inertial sensor signals (**208**). The PPG spectrum and inertial data spectrum, for example, may be obtained by converting the time domain representation to a frequency domain representation using a Fast Fourier Transform.

Peaks in each PPG spectrum are eliminated using the inertial data spectrum from a corresponding window (**210**). For example, peaks in the PPG spectrum that have the same frequency as peaks in the inertial data spectrum may be assumed to be noise caused by movement of the user and therefore may be removed from the PPG spectrum. More than one peak may remain, however. Heart rate candidates are determined from remaining peaks in each PPG spectrum and the heart rate candidates are stored (**212**). The heart rate candidates may be determined from the remaining peaks in each PPG spectrum by performing blind source separation on the PPG signals in the time domain using the inertial data spectrum and the PPG spectrum to reduce a number of the remaining peaks to produce a subset of the remaining peaks, wherein the subset of the remaining peaks are the heart rate candidates. For example, noise removal may be performed by notching out frequencies that appear in the inertial data spectrum and the PPG signal may be additionally filtered with blind source separation using the inertial data spectrum. Blind source separation is a well-known signal processing technique in which source signals are separated from a set of mixed signals where there is little or no information about the source signals or the mixing process. Examples of blind source separation, any of which may be used herein, include, principal components analysis; independent component analysis; dependent component analysis; non-negative matrix factorization; low-complexity coding and decoding; stationary subspace analysis; and common spatial pattern.

A heart rate candidate is selected and the heart rate of the user is tracked based on the heart rate candidate that is selected (**214**). For example, the heart rate candidate may be

selected as a primary peak within the subset of the remaining peaks. Alternatively, the heart rate candidate may be selected as the only remaining peak in the subset of the remaining peaks.

Referring back to FIG. 3, a correlation is determined for heart rate candidates in each new window of PPG spectrum to the heart rate candidates that are stored while the heart rate of the user is continually tracked based on the heart rate candidate that is selected (**216**). A new heart rate candidate is selected from the heart rate candidates that are stored based on the correlation of heart rate candidates and the heart rate of the user is tracked based on the new heart rate candidate that is selected (**218**).

The correlation between heart rate candidates in each new window of PPG spectrum to the stored heart rate candidates may be determined using a frequency tracker for non-stationary harmonic signals. Tracking non-stationary harmonic signals is a known signal processing method typically used in speech analysis, e.g., in pitch detection algorithms. For example, pitch detection is generally discussed in Stephen A. Zahorian and Hongbing Hu, "A Spectral/temporal method for Robust Fundamental Frequency Tracking," The Journal of the Acoustical Society of America, 123 (6), 2008, which is incorporated herein by reference. By way of example, FIG. 4 illustrates a number of PPG spectra over five consecutive windows. Each spectrum includes a plurality of peaks, each of which is a heart rate candidate, and the peak **280** with the star corresponds to the actual heart rate value. Each new spectrum that is generated for a window is correlated to the previous spectra. If the incorrect peak, e.g., peak **282** with the square were selected as the heart rate, tracking would be based on the peak **282**. By determining a correlation for heart rate candidates in each new window of PPG spectrum to the previously stored heart rate candidates, while continually tracking the heart rate, the correct heart rate value, e.g., peak **280**, may eventually be determined and selected as the new heart rate value to be used to track the heart rate. For example, after several windows, there will be a poor correlation between heart rate candidates that are due to noise. As illustrated in FIG. 4, while the first three windows of spectra include the peak **282**, which is due to noise, eventually the peak **282** is no longer present in spectrum. On the other hand, the peak **280** that corresponds to the actual heart rate value is well correlated over multiple windows of spectra. It should be noted that because heart rates change over time, the correlation between heart rate candidates in windows must account for the non-stationary frequency of the heart rate. Thus, the peak **282** may be selected as the new heart rate candidate and the heart rate is tracked based on peak **282**. The selection of a new heart rate candidate may occur, e.g., when the determined correlation for the new heart rate candidate is better than the correlation for a previously selected heart rate candidate. For example, a correlated candidate that is relatively close, e.g., within a set threshold, from the previously selected frequency, may be selected as the new heart rate candidate. For example, a reasonable value for such a threshold is the maximum change of a heart rate within the time of a sliding window, e.g., 8 bpm if the window slides every 2 seconds.

FIG. 5 is a flow chart illustrating a process of resetting the heart rate monitoring by the processor **130** in accordance with another implementation. The method of FIG. 5 is similar to the method described in FIG. 3 discussed above. As illustrated, PPG signals from PPG sensor **110** worn by a user are received (**302**). Additionally, inertial sensor signals from an inertial sensor **120**, which may be accelerometers, worn by the user are received (**304**). The PPG sensor and

inertial sensor are worn on the wrist of the user. The PPG signals and the inertial sensor signals are windowed (306). In other words, a sliding time window of T seconds is applied to the PPG signals and the inertial sensor signals. A PPG spectrum and inertial data spectrum are generated for each window of the PPG signals and inertial sensor signals (308). The PPG spectrum and inertial data spectrum, for example, may be obtained by converting the time domain representation to a frequency domain representation using a Fast Fourier Transform.

Peaks in each PPG spectrum are eliminated using the inertial data spectrum from a corresponding window (310). For example, peaks in the PPG spectrum that have the same frequency as peaks in the inertial data spectrum may be removed from the PPG spectrum. More than one peak may remain, however. One of multiple peaks in a PPG spectrum is selected as an initial value of the heart rate of the user (314). Additionally, blind source separation may be performed on the PPG signals in a time domain using the inertial data spectrum and the PPG spectrum to further reduce the number of the remaining peaks to produce a subset of the remaining peaks, wherein the initial value of the heart rate is selected from the subset of the remaining peaks (312).

The heart rate of the user is tracked based on the initial value of the heart rate (316). Each new PPG spectrum is monitored for an occurrence of a single peak while continuing to track the heart rate of the user based on the peak that was previously selected (318). The heart rate monitoring may be reset by selecting the single peak when the single peak occurs in consecutive PPG spectra as a new value of the heart rate (320). For example, if the single peak occurs in five consecutive PPG spectra, the single peak may be selected as the new value of the heart rate. The heart rate of the user is tracked based on the new value of the heart rate (322).

FIG. 6 is an architecture diagram for the heart rate monitor 100. As illustrated, the PPG sensor 110 and inertial sensor 120, which may be an accelerometer and is labeled ACC, provide signals to a sliding window 402. The sliding window 402 windows the data from the PPG sensor 110 and inertial sensor 120 so that data is separated into windows of T seconds, e.g., 2 seconds, that increment every S seconds, e.g., 2 seconds. Of course, smaller or larger windows may be used and the windows may overlap if desired, where a large overlap permits reporting heart rates more frequently but requires additional computations, and a small overlap permits less computations but heart rates are reported less frequently. The sliding window 402 produces windowed PPG signals $ppg(n)$ and inertial sensor signals $acc(n)$, which are provided to a band pass filter (BPF) 404. The band pass filter 404 passes only a desired band of the PPG signals and inertial sensor signals to remove noise that is outside the frequency band of interest, e.g., between 0.8 Hz and 3.3 Hz.

After the band pass filter 404, the PPG signals $ppg(n)$ and inertial sensor signals $acc(n)$ are provided to a blind source separation filter 406, which filters out the noise. The blind source separation filter 406 filters out the noise by decomposing the time domain PPG sensor signals $ppg(n)$ into a number of simplified time domain signals. The spectrum for each simplified signal are computed and are used along with an inertial data spectrum $ACC(f)$ produced by spectrum estimator 408, to identify the signals that have noise characteristics. The blind source separation filter 406 reduces the number of the remaining peaks by eliminating those simplified signals that have noise characteristics. The blind source separation filter 406 then uses the remaining simplified

signals them to reconstruct the original PPG signal, the spectrum for which will contain a subset of the remaining peaks in the PPG sensor signals. If desired, the blind source separation filter 406 may additionally use the PPG spectrum $PPG(f)$ produced by spectrum estimator 408, the current heart rate HR from heart rate converter 414, and the trends in the PPG signals and the inertial sensor signals (ppg and acc trends) from the trend estimator 424, to identify and remove noise.

FIG. 7, by way of example, illustrates the operation of the blind source separation filter 406. As can be seen, the blind source separation filter 404 receives the PPG signal 502 and decomposes 504 the time domain PPG signal into a plurality of more simple decomposed signals 506, e.g., using singular value decomposition or a similar technique, which are converted into spectra 510 in the frequency domain, e.g., using a Fast Fourier Transform 508. Noise characteristics in identified and removed 512 by comparing each spectrum in spectra 510 to the inertial data spectrum $ACC(f)$ produced by spectrum estimator 408 and eliminating any spectrum that has noise characteristics, i.e., have peaks that within a threshold amount from the inertial data spectrum $ACC(f)$, resulting in spectra 514. For example, the threshold may be within 2 frequency bins of the inertial data spectrum $ACC(f)$ peaks. The simple decomposed signals 506 that correspond to the remaining spectra 514 are recombined 516 to reconstruct the PPG signal 518, but with peaks corresponding to noise removed.

The blind source separation filter 406 identifies noise by comparing the inertial data spectrum $ACC(f)$, produced by the spectrum estimator 408, to the decomposed signals and eliminates peaks in the PPG sensor signals that are the same or nearly the same as dominant peaks in the inertial data spectrum $ACC(f)$. If, however, a dominant peak in the inertial sensor spectrum $ACC(f)$ matches the previous heart rate HR, as provided by heart rate converter 414, that peak is not removed from the PPG sensor signals.

If desired, additional noise criteria may be used in the blind source separation filter 406 to identify and remove noise from the PPG sensor signals. For example, the maximum singular value may be observed and used as a threshold to eliminate anything less, e.g., any peaks less than 1% of max value may be removed. For example, the spectrum 510 associated with a simple decomposed signal 506, shown in FIG. 7, may be associated with a singular value. The simple decomposed signals having a spectrum with a small singular value, e.g., less than 1% of the maximum singular value, may be eliminated.

Additionally, if there are more than two dominant peaks in the spectrum 510 of the simple decomposed signals 506, the blind source separation filter 406 may eliminate those signals. Dominant peaks may be determined, e.g., as any peak that is greater than a designated percentage of the maximum peak, e.g., 90%.

Additionally, the blind source separation filter 406 may eliminate peaks in the PPG sensor signals using a threshold that is based on a maximum possible change in a heart rate within specific period of time. For example, in general, it is unlikely that a heart rate will change more than 10 beats/min within a 2 second window. Accordingly, if a peak in the PPG sensor signals represents a frequency (or heart rate) that is more than a threshold amount from the previous heart rate HR, as provided by heart rate converter 414, the peak may be eliminated. Additionally, because the previous heart rate HR may not be correct, the blind source separation filter 406 may compare peaks in the PPG sensor signals to an average heart rate determined based on the previous heart rate HR

and the peaks in the PPG spectrum $ACC(f)$ as provided by the spectrum estimator **408**, that are closest to the previous heart rate HR . For example, an average heart rate $\bar{N}$ as

$$\bar{N} = \frac{N_{prev} + N_{new}}{2} \quad \text{eq. 1}$$

where N_{prev} is the previous heart rate and N_{new} is an average of the closest peaks in the PPG spectrum $ACC(f)$ to the previous heart rate N_{prev} , e.g., where peaks are considered close if they are within a threshold amount from the previous heart rate N_{prev} .

Additionally, the blind source separation filter **406** may eliminate peaks in the PPG sensor signals if the peaks are not consistent with the ppg trend as provided by the trend estimator **424**. In other words, if the trend estimator **424** estimates that the heart rate is increasing, then the blind source separation filter **406** may eliminate any peaks in the PPG sensor signals that are less than a threshold from the previous heart rate HR , e.g., 3 bpm or less than the previous estimated heart rate HR . Similarly, if the trend estimator **424** estimates that the heart rate is decreasing, then the blind source separation filter **406** may eliminate any peaks in the PPG sensor signals that are more than a threshold from the previous heart rate HR .

Additional, fewer or different criteria for identifying and removing noise from the PPG sensor signals may be used by the blind source separation filter **406** if desired. After the noise is identified and removed from the decomposed signals, the decomposed signals are recombined to produce the PPG sensor single $ppg(n)$ with peaks corresponding to noise removed.

The resulting PPG sensor single $ppg(n)$ is received by the spectrum estimator **408**, which also receives the inertial sensor signal $acc(n)$. The spectrum estimator **408** converts the PPG sensor single $ppg(n)$ and the inertial sensor signal $acc(n)$ in each window into the frequency domain PPG spectrum $PPG(f)$ and inertial data spectrum $ACC(f)$, respectively, e.g., using a Fast Fourier Transform. The remaining peaks in the resulting PPG spectrum $PPG(f)$ in each window are the heart rate candidates and are provided to the adaptive spectrum peak tracker **410**. The resulting PPG spectrum $PPG(f)$ may also be provided to the blind source separation filter **406** along with the resulting inertial data spectrum $ACC(f)$.

The adaptive spectrum peak tracker **410** receives the PPG spectrum $PPG(f)$ from the spectrum estimator **408**, as well as the current heart rate HR from heart rate converter **414**, and the trends in the PPG signals and the inertial sensor signals (ppg and acc trends) from the trend estimator **424**. The PPG spectrum $PPG(f)$ in each window may include more than one peak, i.e., there may be multiple heart rate candidates. The adaptive spectrum peak tracker **410** may select one of the peaks as corresponding to the heart rate, and thus, is the frequency of the heart rate N_f . The adaptive spectrum peak tracker **410** may select a peak from the PPG spectrum $PPG(f)$, e.g., by comparing peaks from the inertial data spectrum $ACC(f)$ and the PPG spectrum $PPG(f)$ over multiple windows, and determining which peak in the PPG spectrum $PPG(f)$ corresponds to the heart rate peak and which peaks correspond to noise. Additionally, the adaptive spectrum peak tracker **410** may eliminate heart rate candidates that are not consistent with the heart rate trend as provided by the trend estimator **424**. In other words, if the trend estimator **424** estimates that the heart rate is increasing,

then the adaptive spectrum peak tracker **410** may eliminate any heart rate candidates that are less than a threshold from the previous heart rate HR , e.g., 3 bpm or less than the previous estimated heart rate HR . Similarly, if the trend estimator **424** estimates that the heart rate is decreasing, then the adaptive spectrum peak tracker **410** may eliminate any heart rate candidates that are more than a threshold from the previous heart rate HR .

The selected value of the heart rate N_f may be used to track the heart rate of the user. However, the adaptive spectrum peak tracker **410** may reset the value of the heart rate N_f if it determines that the previously selected value is incorrect. For example, as discussed in reference to FIG. 5, each new PPG spectrum $PPG(f)$ is monitored for an occurrence of a single peak, while the heart rate of the user is continually tracked based on a previously selected value of the heart rate N_f . If a single peak occurs over a number of consecutive windows, e.g., five consecutive windows, the heart rate may be reset by selecting the single peak as the new value of the heart rate.

The selected value of the heart rate N_f is provided to a feasibility checker **412**, which also receives the current heart rate HR from heart rate converter **414**, and the trends in the PPG signals and the inertial sensor signals (ppg and acc trends) from the trend estimator **424**. The feasibility checker **412** determines whether the selected value of the heart rate N_f is feasible and may reset the value for the heart rate N_f if it determines that the selected value of the heart rate N_f is incorrect. For example, as discussed in reference to FIG. 3, the heart rate of the user may be continually tracked while the feasibility checker **412** may determine a correlation for heart rate candidates, i.e., peaks, in each new window of spectrum $PPG(f)$ to the heart rate candidates from previous windows. If a non-selected heart rate candidate is determined to have a better correlation with heart rate candidates from previous windows, the feasibility checker **412** may switch the value of the heart rate N_f to the heart rate candidate with the better correlation.

The selected value of the heart rate N_f is provided to the heart rate converter **414**. The heart rate converter **414** converts the final selected frequency of the heart rate N_f to a heart rate HR by scaling it. The current value of the heart rate HR is provided to the blind source separation filter **406**, the adaptive spectrum peak tracker **410**, the feasibility checker **412**, as well as the pipeline **420**.

The smoother **416** receives the heart rate HR from the pipeline **420** and smoothes the heart rate HR , e.g., using a low pass filter or a median filter on the last K reported HR values, e.g., K may be 10. The smoother **416** provides the reported heart rate **418**, which may be displayed to the user, or provided to other applications on the heart rate monitor **100** or a remote device, e.g., using wireless communications, such as Blue Tooth or the like.

The heart rate HR is further provided from the pipeline **420** to the trend estimator **424**. The trend estimator **424** additionally receives the inertial sensor signals $acc(n)$ after passing through a low pass filter **426**. The low pass filter **426** keeps only low frequency components in the inertial sensor signals $acc(n)$, e.g., less than 0.2 Hz. The trend estimator **424** uses the inertial sensor signals and the previous history of the heart rate HR to determine the trends in the inertial sensor data and the heart rate, e.g., whether user movement is increasing, decreasing or staying the same and whether the user heart rate is increasing, decreasing or staying the same. The trend may be found, e.g., by determining the slope of the last M values of the heart rate HR or inertial sensor signals, wherein if the slope is positive, the trend is upward, if the

slope is negative, the trend is downward, and if the slope is zero, the trend is flat. The trends in the PPG signals, i.e., heart rate, and the inertial sensor signals (ppg and acc trends) is provided to the blind source separation filter **406**, the adaptive spectrum peak tracker **410** and the feasibility checker **412**, as discussed above.

FIG. **8** is a block diagram of the heart rate monitor **100**, which is wrist worn by the user and includes a PPG sensor **110**, multiple axis inertial sensor **120**, and processor **130** as discussed herein. The PPG sensor **110** may be an optical PPG sensor. The multiple axis inertial sensor **120** may include two or three axes and may be, for example, a three axis accelerometer, gyroscopes, or the like. The heart rate monitor **100** further includes a user interface **102** that may include, e.g., a display, as well as a real or virtual keys or other input device through which the user may, e.g., input information, make selections.

As illustrated, the PPG sensor **110**, inertial sensor **120**, and user interface **102** are coupled to the processor **130**, e.g., a bus **122**. Thus, the processor **130** is connected to receive signals from the PPG sensor **110** and the inertial sensor **120** and to communicate with the user interface **102**. The processor **130** is further connected to memory **132**, e.g., via the bus **122**. The processor **130** is configured to receive and processes the signals from the PPG sensor **110** and inertial sensor **120** as described herein. For example, the architecture discussed in FIG. **6** may be implemented within processor **130**. It should be understood, however, that the particular architecture used in the heart rate monitor **100** may vary if desired. The methodologies described herein may be implemented by various means depending upon the application. For example, the processor **130** may implement the methodologies discussed herein using hardware, firmware or software. For example, the architecture discussed in FIG. **6** may be implemented in the processor **130** based on instructions in software or firmware which may be stored in memory **132** and run in the processor **130**. Further, it should be understood that the processor **130** may be one or more processors operating together to perform the functions discussed herein.

For example, the processor **130** may, but need not necessarily include, one or more microprocessors, embedded processors, controllers, application specific integrated circuits (ASICs), digital signal processing devices (DSPDs), programmable logic devices (PLDs), field programmable gate arrays (FPGAs), and the like. Moreover, as used herein the term "memory" refers to any type of computer storage medium, including long term, short term, or other memory associated with the mobile device, and is not to be limited to any particular type of memory or number of memories, or type of media upon which memory is stored.

For a firmware and/or software implementation, the methodologies may be implemented with modules (e.g., procedures, functions, and so on) that perform the functions described herein. Any machine-readable medium tangibly embodying instructions may be used in implementing the methodologies described herein. For example, software codes may be stored in memory **132** and executed by the processor **130**. Memory **132m** may be implemented within or external to the processor **130**. If implemented in firmware and/or software, the functions may be stored as one or more instructions or code on a computer-readable medium. Examples include non-transitory computer-readable media encoded with a data structure and computer-readable media encoded with a computer program. Computer-readable media includes physical, i.e., non-transitory, computer storage media. A storage medium may be any available medium

that can be accessed by a computer. By way of example, and not limitation, such computer-readable media can comprise RAM, ROM, EEPROM, CD-ROM or other optical disk storage, magnetic disk storage or other magnetic storage devices, or any other medium that can be used to store desired program code in the form of instructions or data structures and that can be accessed by a computer; disk and disc, as used herein, includes compact disc (CD), laser disc, optical disc, digital versatile disc (DVD), floppy disk and Blu-ray disc where disks usually reproduce data magnetically, while discs reproduce data optically with lasers. Combinations of the above should also be included within the scope of computer-readable media.

Although the present invention is illustrated in connection with specific embodiments for instructional purposes, the present invention is not limited thereto. Various adaptations and modifications may be made without departing from the scope of the invention. Therefore, the spirit and scope of the appended claims should not be limited to the foregoing description.

What is claimed is:

1. A method for monitoring a heart rate, the method comprising:

- receiving photoplethysmogram (PPG) signals from a PPG sensor worn by a user;
- receiving inertial sensor signals from an inertial sensor worn by the user;
- windowing the PPG signals and the inertial sensor signals;
- generating a PPG spectrum and an inertial data spectrum for each window of the PPG signals and the inertial sensor signals;
- eliminating peaks in each PPG spectrum using the inertial data spectrum from a corresponding window;
- determining a plurality of heart rate candidates from remaining peaks in each PPG spectrum and storing the plurality of heart rate candidates;
- selecting a heart rate candidate and tracking the heart rate of the user based on the heart rate candidate that is selected;
- reporting the tracked heart rate of the user that is based on the heart rate candidate that is selected;
- determining a correlation of heart rate candidates in each new window of PPG spectrum to the plurality of heart rate candidates that are stored while continuing to track the heart rate of the user based on the heart rate candidate that is selected;
- selecting a new heart rate candidate from the plurality of heart rate candidates that are stored based on the correlation of heart rate candidates and tracking the heart rate of the user based on the new heart rate candidate that is selected; and
- reporting the heart rate of the user that is based on the new heart rate candidate that is selected.

2. The method of claim 1, wherein generating the PPG spectrum and the inertial data spectrum comprises converting a time domain representation of PPG signals for each window into a frequency domain representation using a Fast Fourier Transform and converting a time domain representation of inertial sensor signals for each window into a frequency domain representation using the Fast Fourier Transform.

3. The method of claim 1, wherein the PPG sensor and the inertial sensor are worn on a wrist of the user.

4. The method of claim 1, wherein the inertial sensor comprises accelerometers.

11

5. The method of claim 1, wherein determining the plurality of heart rate candidates from the remaining peaks in each PPG spectrum comprises performing blind source separation on the PPG signals in a time domain using the inertial data spectrum and the PPG spectrum to reduce a number of the remaining peaks to produce a subset of the remaining peaks, wherein the subset of the remaining peaks are the plurality of heart rate candidates.

6. The method of claim 5, wherein selecting the heart rate candidate comprises selecting a primary peak or an only remaining peak from the subset of the remaining peaks.

7. The method of claim 1, further comprising determining a heart rate trend and a physical activity trend rate and using them to determine if the heart rate is correct.

8. The method of claim 1, wherein reporting the tracked heart rate of the user comprises at least one of displaying the tracked heart rate to the user, providing the tracked heart rate to an application; wirelessly providing the tracked heart rate to a remote device.

9. A heart rate monitor that is worn by a user and monitors a heart rate of the user, the heart rate monitor comprising:

a photoplethysmogram (PPG) sensor that monitors the user and produces PPG signals;

an inertial sensor that produces inertial sensor signals in response to user motion;

a display for displaying a heart rate of the user;

a processor coupled to receive the PPG signals from the PPG sensor and the inertial sensor signals from the inertial sensor and coupled to the display, the processor being configured to window the PPG signals and the inertial sensor signals, generate a PPG spectrum and an inertial data spectrum for each window of the PPG signals and the inertial sensor signals, eliminate peaks in each PPG spectrum using the inertial data spectrum from a corresponding window, determine a plurality of heart rate candidates from remaining peaks in each PPG spectrum and store the plurality of heart rate candidates, select a heart rate candidate and tracking the heart rate of the user based on the heart rate candidate that is selected, cause the display to display the tracked heart rate of the user that is based on the heart rate candidate that is selected, determine a correlation of heart rate candidates in each new window of PPG spectrum to the plurality of heart rate candidates

12

that are stored while continuing to track the heart rate of the user based on the heart rate candidate that is selected, select a new heart rate candidate from the plurality of heart rate candidates that are stored based on the correlation of heart rate candidates and tracking the heart rate of the user based on the new heart rate candidate that is selected; and cause the display to display the heart rate of the user that is based on the new heart rate candidate that is selected.

10. The heart rate monitor of claim 9, wherein the processor is configured to generate the PPG spectrum and the inertial data spectrum by being configured to convert a time domain representation of PPG signals for each window into a frequency domain representation using a Fast Fourier Transform and convert a time domain representation of inertial sensor signals for each window into a frequency domain representation using the Fast Fourier Transform.

11. The heart rate monitor of claim 9, wherein the PPG sensor and the inertial sensor are configured to be worn on a wrist of the user.

12. The heart rate monitor of claim 9, wherein the inertial sensor comprises accelerometers.

13. The heart rate monitor of claim 9, wherein the processor is configured to determine the plurality of heart rate candidates from the remaining peaks in each PPG spectrum by being configured to perform blind source separation on the PPG signals in a time domain using the inertial data spectrum and the PPG spectrum to reduce a number of the remaining peaks to produce a subset of the remaining peaks, wherein the subset of the remaining peaks are the plurality of heart rate candidates.

14. The heart rate monitor of claim 13, wherein the processor is configured to select the heart rate candidate by being configured to select a primary peak or an only remaining peak from the subset of the remaining peaks.

15. The heart rate monitor of claim 9, wherein the processor is further configured to determine a heart rate trend and a physical activity trend rate and using them to determine if the heart rate is correct.

16. The heart rate monitor of claim 9, wherein the processor is further configured to provide the tracked heart rate to an application or wirelessly provide the tracked heart rate to a remote device.

* * * * *

专利名称(译)	心率监测器		
公开(公告)号	US10456053	公开(公告)日	2019-10-29
申请号	US15/054022	申请日	2016-02-25
申请(专利权)人(译)	QuickLogic公司		
当前申请(专利权)人(译)	QuickLogic公司		
[标]发明人	EMADZADEH AMIR ABBAS		
发明人	EMADZADEH, AMIR ABBAS		
IPC分类号	A61B5/024 A61B5/00		
CPC分类号	A61B5/7207 A61B5/681 A61B5/02438 A61B5/6824 A61B5/7275 A61B5/7282		
优先权	62/195730 2015-07-22 US		
其他公开文献	US20170020398A1		
外部链接	Espacenet		

摘要(译)

腕戴式心率监测器包括光电容积描记 (PPG) 传感器和惯性传感器。来自惯性传感器的信号用于识别和消除PPG信号中的噪声。从保留在所得PPG频谱中的多个候选心率中选择初始心率值，并将其用于跟踪用户的心率。在跟踪心率时监测PPG频谱，以确定所选的初始心率值是否有误。可以通过确定每个PPG频谱中可能的心率候选者与先前的心率候选者之间的相关性并相应地重置心率值来监视PPG频谱。另外地或可替代地，可以通过确定在连续的PPG频谱中何时仅存在单个心率候选者并相应地重置心率值来监视PPG频谱。

