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(54) ULTRASONIC BLOOD PRESSURE MEASURING DEVICE AND ULTRASONIC BLOOD PRESSURE MEASURING METHOD

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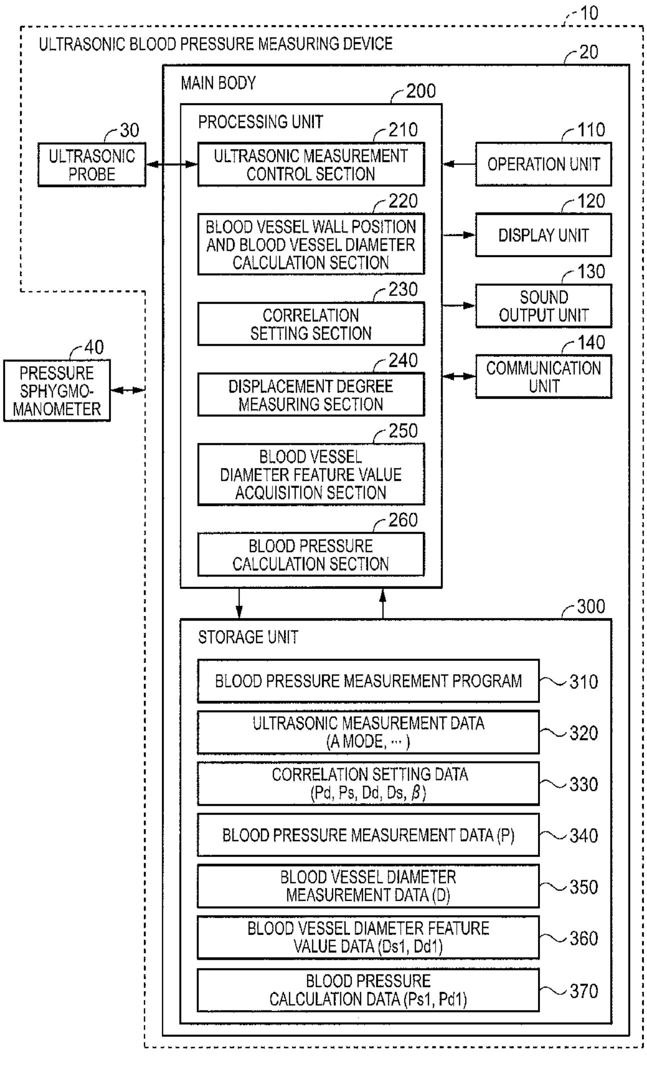
(57) ABSTRACT

An ultrasonic blood pressure measuring device receives a reflected wave of an ultrasonic wave transmitted to a blood vessel, and measures the degree of displacement of a blood vessel wall of the blood vessel based on the reflected wave of the ultrasonic wave during at least one heartbeat period. Then, cardiac systolic blood pressure and cardiac diastolic blood pressure are calculated from a maximum value of the blood vessel diameter, which appears after the peak of the degree of displacement of the blood vessel wall, and a minimum value of the blood vessel diameter, which appears before the peak, using a correlation between the diameter of blood vessel and blood pressure set in advance.



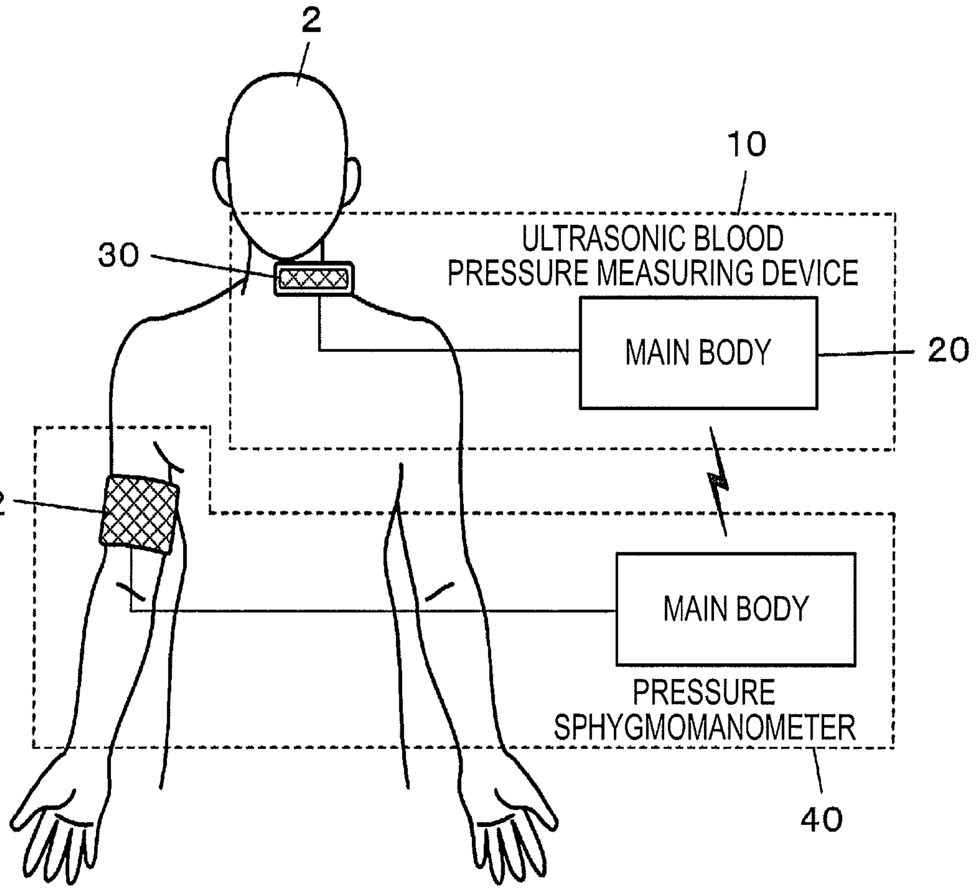

2
10
ULTRASONIC BLOOD PRESSURE MEASURING DEVICE
30
MAIN BODY
20
42
MAIN BODY
PRESSURE SPHYGMOMANOMETER
40

FIG. 1

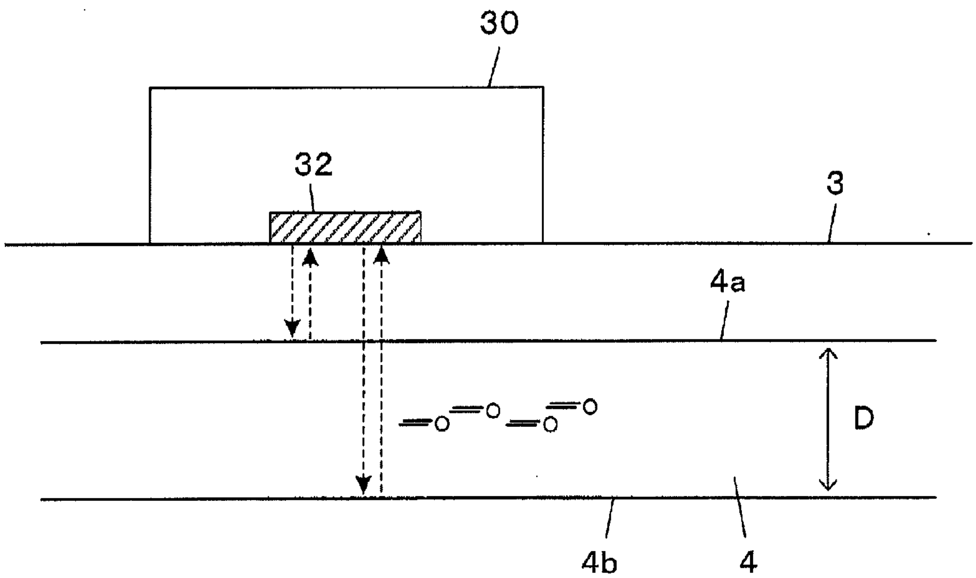


FIG. 2

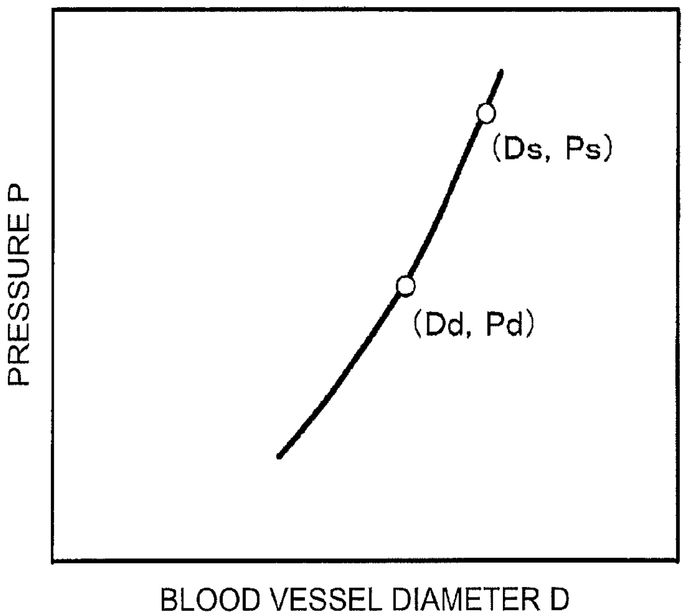


FIG. 3

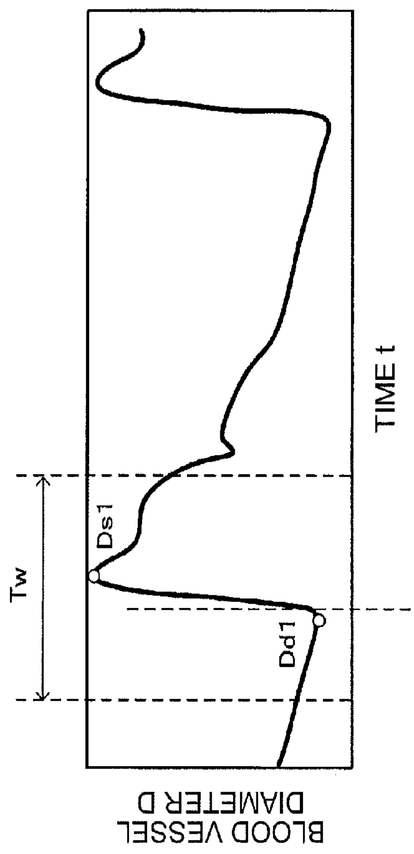

Tw
Ds1
Dd1
BLOOD VESSEL DIAMETER D
TIME t

FIG. 4A

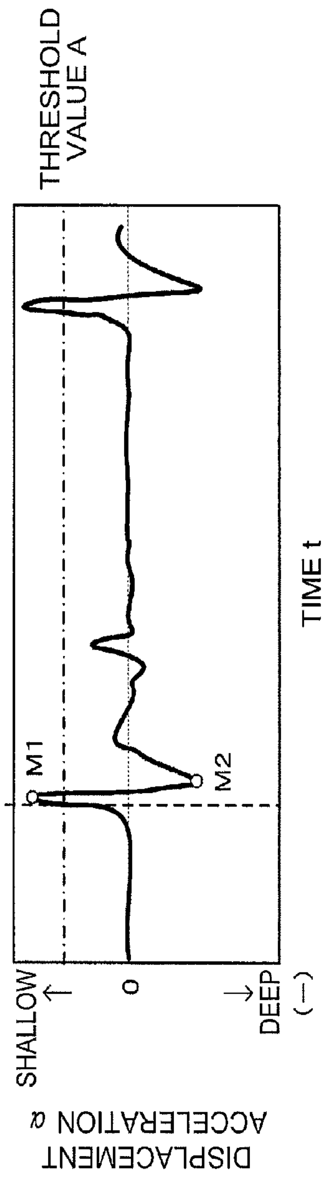

THRESHOLD VALUE A
M1
M2
(+) SHALLOW ↑
0
↓ DEEP (−)
DISPLACEMENT ACCELERATION α
TIME t

FIG. 4B

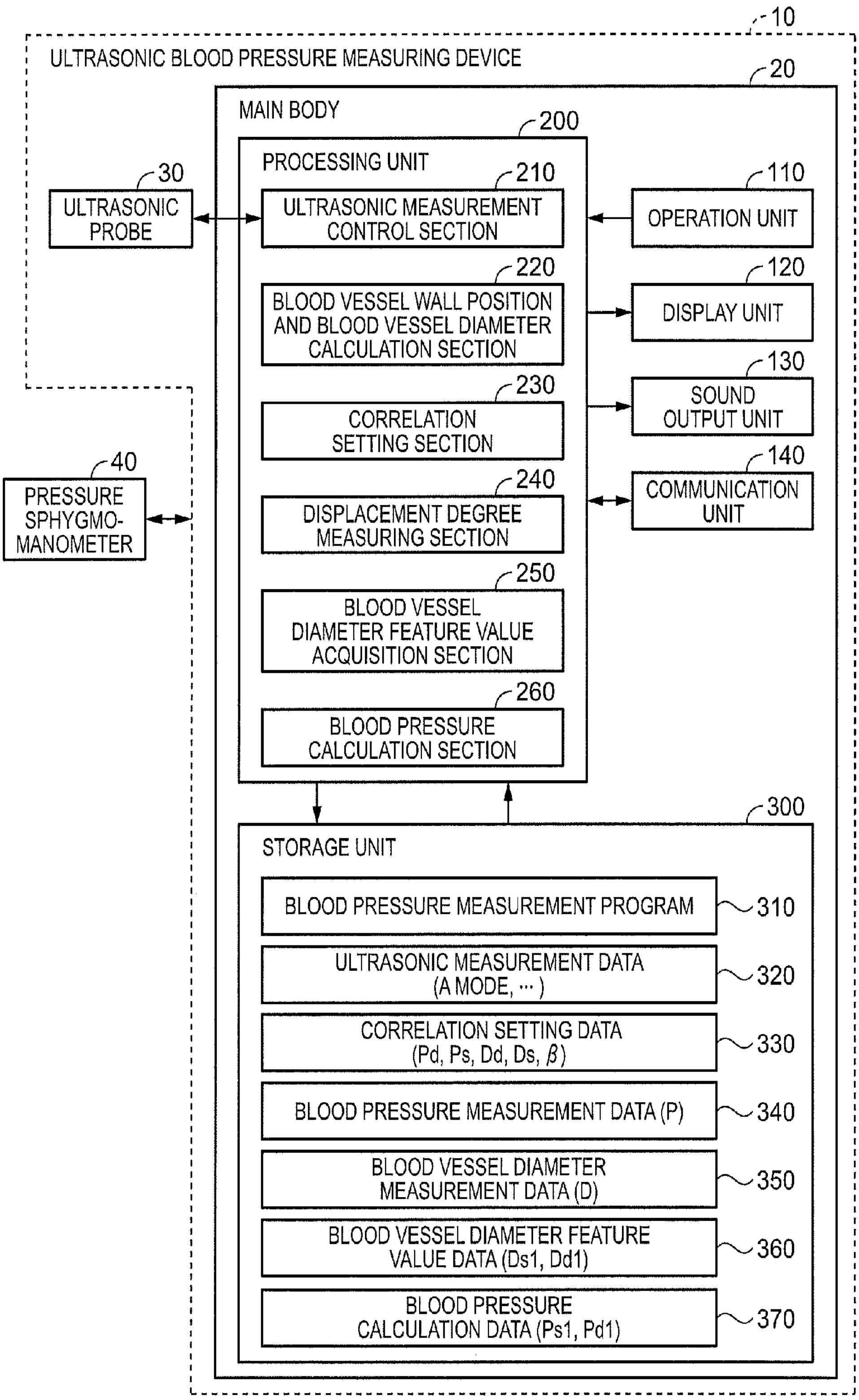

10
ULTRASONIC BLOOD PRESSURE MEASURING DEVICE
20
MAIN BODY
200
PROCESSING UNIT
30
ULTRASONIC PROBE
210
ULTRASONIC MEASUREMENT CONTROL SECTION
110
OPERATION UNIT
220
BLOOD VESSEL WALL POSITION AND BLOOD VESSEL DIAMETER CALCULATION SECTION
120
DISPLAY UNIT
130
SOUND OUTPUT UNIT
230
CORRELATION SETTING SECTION
40
PRESSURE SPHYGMO-MANOMETER
240
DISPLACEMENT DEGREE MEASURING SECTION
140
COMMUNICATION UNIT
250
BLOOD VESSEL DIAMETER FEATURE VALUE ACQUISITION SECTION
260
BLOOD PRESSURE CALCULATION SECTION
300
STORAGE UNIT
BLOOD PRESSURE MEASUREMENT PROGRAM
310
ULTRASONIC MEASUREMENT DATA (A MODE, ···)
320
CORRELATION SETTING DATA (Pd, Ps, Dd, Ds, β)
330
BLOOD PRESSURE MEASUREMENT DATA (P)
340
BLOOD VESSEL DIAMETER MEASUREMENT DATA (D)
350
BLOOD VESSEL DIAMETER FEATURE VALUE DATA (Ds1, Dd1)
360
BLOOD PRESSURE CALCULATION DATA (Ps1, Pd1)
370

FIG. 5

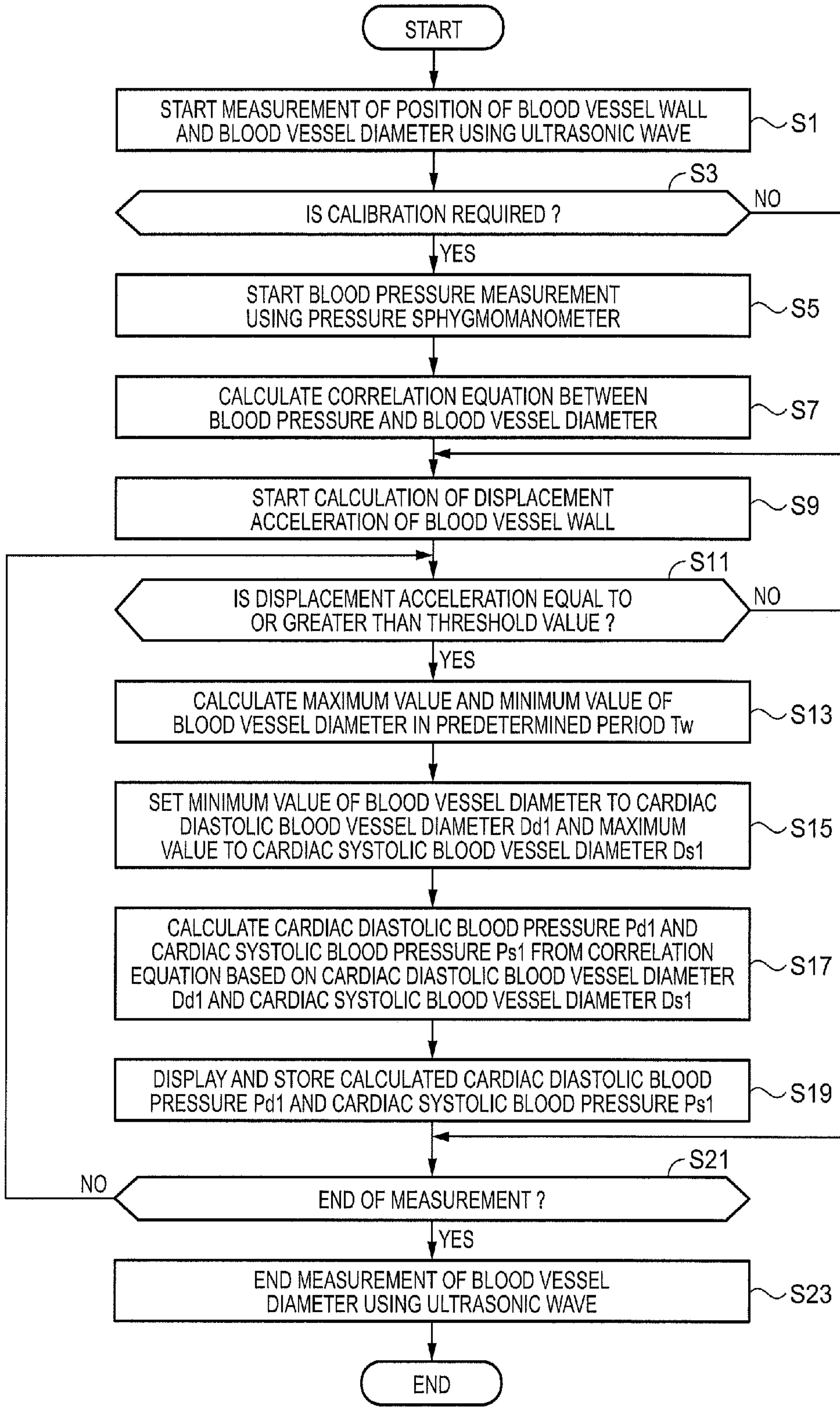

START
START MEASUREMENT OF POSITION OF BLOOD VESSEL WALL AND BLOOD VESSEL DIAMETER USING ULTRASONIC WAVE
S1
S3
IS CALIBRATION REQUIRED ?
NO
YES
START BLOOD PRESSURE MEASUREMENT USING PRESSURE SPHYGMOMANOMETER
S5
CALCULATE CORRELATION EQUATION BETWEEN BLOOD PRESSURE AND BLOOD VESSEL DIAMETER
S7
START CALCULATION OF DISPLACEMENT ACCELERATION OF BLOOD VESSEL WALL
S9
S11
IS DISPLACEMENT ACCELERATION EQUAL TO OR GREATER THAN THRESHOLD VALUE ?
NO
YES
CALCULATE MAXIMUM VALUE AND MINIMUM VALUE OF BLOOD VESSEL DIAMETER IN PREDETERMINED PERIOD Tw
S13
SET MINIMUM VALUE OF BLOOD VESSEL DIAMETER TO CARDIAC DIASTOLIC BLOOD VESSEL DIAMETER Dd1 AND MAXIMUM VALUE TO CARDIAC SYSTOLIC BLOOD VESSEL DIAMETER Ds1
S15
CALCULATE CARDIAC DIASTOLIC BLOOD PRESSURE Pd1 AND CARDIAC SYSTOLIC BLOOD PRESSURE Ps1 FROM CORRELATION EQUATION BASED ON CARDIAC DIASTOLIC BLOOD VESSEL DIAMETER Dd1 AND CARDIAC SYSTOLIC BLOOD VESSEL DIAMETER Ds1
S17
DISPLAY AND STORE CALCULATED CARDIAC DIASTOLIC BLOOD PRESSURE Pd1 AND CARDIAC SYSTOLIC BLOOD PRESSURE Ps1
S19
S21
NO
END OF MEASUREMENT ?
YES
END MEASUREMENT OF BLOOD VESSEL DIAMETER USING ULTRASONIC WAVE
S23
END

FIG. 6

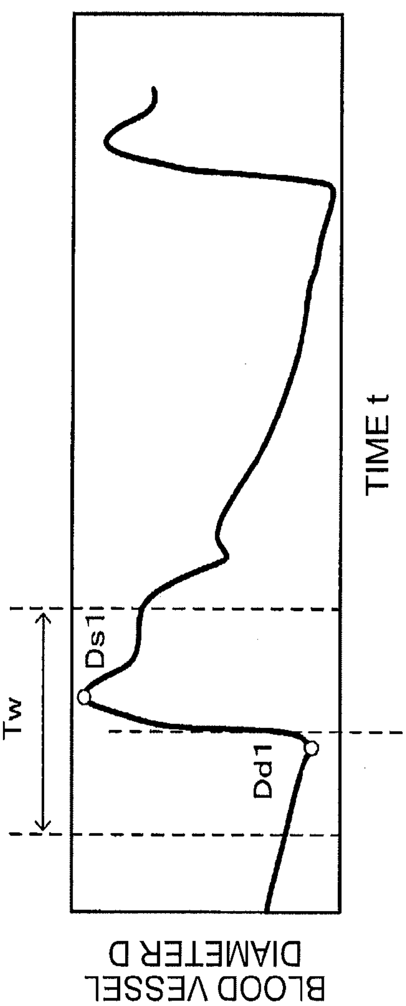

BLOOD VESSEL DIAMETER D
TIME t
Tw
Ds1
Dd1

FIG. 7A

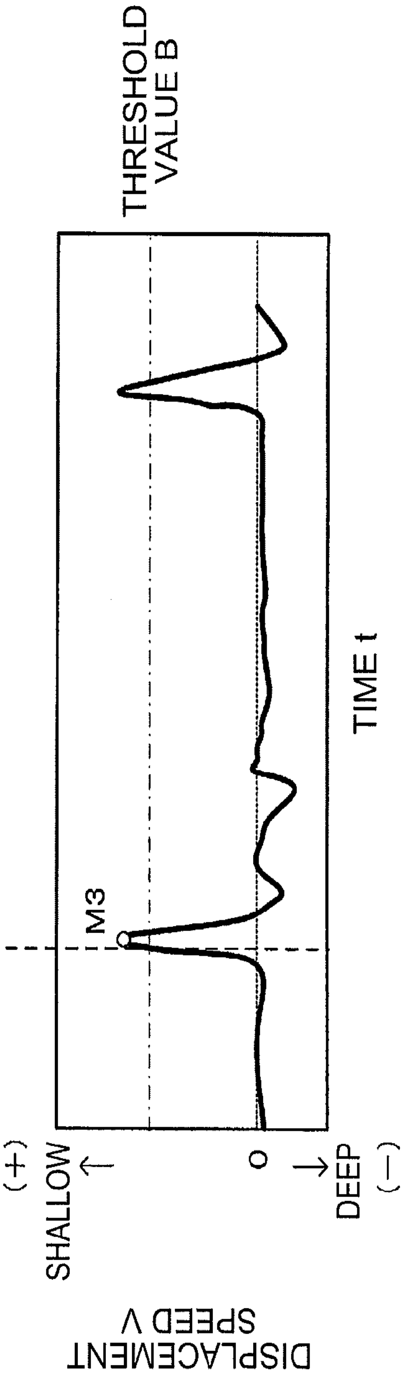

THRESHOLD VALUE B
TIME t
M3
DISPLACEMENT SPEED V
SHALLOW
(+)
o
DEEP
(−)

FIG. 7B

BLOOD VESSEL DIAMETER (mm)	BLOOD PRESSURE (mmHg)
XXXX	XXXX
XXXX	XXXX
⋮	⋮

FIG. 8

ULTRASONIC BLOOD PRESSURE MEASURING DEVICE AND ULTRASONIC BLOOD PRESSURE MEASURING METHOD

BACKGROUND

[0001] 1. Technical Field

[0002] The present invention relates to an ultrasonic blood pressure measuring device that measures blood pressure using an ultrasonic wave.

[0003] 2. Related Art

[0004] As a method for measuring the blood pressure of a subject in a non-invasive manner, a technique of measuring the diameter of the blood vessel of a subject using an ultrasonic wave and estimating the blood pressure from the blood vessel diameter is known. For example, JP-A-2004-41382 discloses a method of regarding the relationship between the blood vessel diameter and blood pressure as a non-linear function and calculating the blood pressure from the blood vessel diameter and a stiffness parameter β indicating the hardness of the blood vessel.

[0005] In general, in blood pressure measurement, the highest blood pressure (cardiac systolic blood pressure) and the lowest blood pressure (cardiac diastolic blood pressure) are measured. That is, when calculating the blood pressure using the relationship between the blood vessel diameter and blood pressure as described above, a cardiac systolic blood vessel diameter that is a blood vessel diameter at the time of the highest blood pressure (cardiac systolic blood pressure) and a cardiac diastolic blood vessel diameter that is a blood vessel diameter at the time of the lowest blood pressure (cardiac diastolic blood pressure) need to be measured first.

[0006] In a cuff type pressure sphygmomanometer used in known blood pressure measurement, there is a disadvantage in that about tens of seconds are required for measurement and continuous measurement is not possible. Therefore, quick and continuous blood pressure measurement has been demanded.

SUMMARY

[0007] An advantage of some aspects of the invention is to enable quick and continuous measurement of the highest blood pressure (cardiac systolic blood pressure) and the lowest blood pressure (cardiac diastolic blood pressure) in blood pressure measurement using an ultrasonic wave.

[0008] A first aspect of the invention is directed to an ultrasonic blood pressure measuring device including: a transmission and reception unit that transmits an ultrasonic wave to a blood vessel and receives a reflected wave of the ultrasonic wave; a displacement degree measuring unit that measures a degree of displacement of a blood vessel wall of the blood vessel based on reflected wave of the ultrasonic wave during at least one heartbeat period; a blood vessel diameter measuring unit that measures a diameter of the blood vessel based on the reflected wave; a peak calculation unit that calculates a peak of the degree of displacement of the blood vessel wall; a blood vessel diameter acquisition unit that acquires a maximum value of the blood vessel diameter, which appears after the peak of the degree of displacement of the blood vessel wall, as a cardiac systolic blood vessel diameter and acquires a minimum value of the blood vessel diameter, which appears before the peak, as a cardiac diastolic blood vessel diameter; and a blood pressure calculation unit that calculates cardiac systolic blood pressure and cardiac diastolic blood pressure from the cardiac systolic blood vessel diameter and the cardiac diastolic blood vessel diameter using a correlation between the diameter of the blood vessel and blood pressure set in advance.

[0009] As another aspect of the invention, the invention may be configured as an ultrasonic blood pressure measuring method including: receiving a reflected wave of an ultrasonic wave transmitted to a blood vessel and measuring a degree of displacement of a blood vessel wall of the blood vessel based on the reflected wave of the ultrasonic wave during at least one heartbeat period; measuring a diameter of the blood vessel based on the reflected wave; calculating a peak of the degree of displacement of the blood vessel wall; and calculating cardiac systolic blood pressure and cardiac diastolic blood pressure from a maximum value of the blood vessel diameter, which appears after the peak of the degree of displacement of the blood vessel wall, and a minimum value of the blood vessel diameter, which appears before the peak, using a correlation between the diameter of the blood vessel and blood pressure set in advance.

[0010] According to the first aspect and the like of the invention, it is possible to measure the cardiac systolic blood pressure and the cardiac diastolic blood pressure for each heartbeat. The blood vessel repeats expansion and contraction due to the beating of the heart, and the position (depth position) of the blood vessel wall changes according to the expansion and contraction. For example, the artery has a feature that the change in the position of the blood vessel wall is fast in cardiac systole but is slow in cardiac diastole. That is, since the degree of displacement of the blood vessel wall in cardiac systole is large compared with that in cardiac diastole, the peak of the degree of displacement of the blood vessel wall appears in cardiac systole. Accordingly, the minimum value of the blood vessel diameter appearing before the peak of the degree of displacement of the blood vessel wall can be acquired as the cardiac diastolic blood vessel diameter, and the maximum value of the blood vessel diameter appearing after the peak of the degree of displacement of the blood vessel wall can be acquired as the cardiac systolic blood vessel diameter. Therefore, since the cardiac systolic blood pressure and the cardiac diastolic blood pressure appearing for each heartbeat can be measured, it is possible to measure the highest blood pressure (cardiac systolic blood pressure) and the lowest blood pressure (cardiac diastolic blood pressure) quickly and continuously.

[0011] As a second aspect of the invention, the ultrasonic blood pressure measuring device according to the first aspect of the invention may be configured such that the displacement degree measuring unit measures a displacement speed of the blood vessel wall as the degree of displacement.

[0012] According to the second aspect of the invention, a displacement speed is measured as the degree of displacement of the blood vessel wall.

[0013] As a third aspect of the invention, the ultrasonic blood pressure measuring device according to the first aspect of the invention may be configured such that the displacement degree measuring unit measures displacement acceleration of the blood vessel wall as the degree of displacement.

[0014] According to the third aspect of the invention, displacement acceleration is measured as the degree of displacement of the blood vessel wall.

[0015] As a fourth aspect of the invention, the ultrasonic blood pressure measuring device according to any one of the first to third aspects of the invention may be configured such that the ultrasonic blood pressure measuring device further includes a correlation setting unit that sets the correlation.

[0016] According to the fourth aspect of the invention, a correlation between the blood vessel diameter and blood pressure is set. The correlation between the blood vessel diameter and blood pressure differs depending on an individual. Therefore, a calibration suitable for a subject can be realized by setting the correlation between the blood vessel diameter and blood pressure using the blood pressure measured separately, for example.

[0017] As a fifth aspect of the invention, the ultrasonic blood pressure measuring device according to any one of the first to fourth aspects of the invention may be configured such that the blood vessel is an artery.

[0018] According to the fifth aspect of the invention, it is possible to measure the blood pressure of the artery.

[0019] As a sixth aspect of the invention, the ultrasonic blood pressure measuring device according to any one of the first to fifth aspects of the invention may be configured such that the ultrasonic blood pressure measuring device further includes a storage unit that stores the correlation as a look-up table of the blood vessel diameter and the blood pressure, and the blood pressure calculation unit calculates cardiac systolic blood pressure and cardiac diastolic blood pressure from the cardiac systolic blood vessel diameter and the cardiac diastolic blood vessel diameter with reference to the look-up table.

[0020] According to the sixth aspect of the invention, it is possible to store the correlation between the blood vessel diameter and blood pressure as a look-up table. Therefore, it is possible to reduce the calculation load when calculating the blood pressure.

BRIEF DESCRIPTION OF THE DRAWINGS

[0021] The invention will be described with reference to the accompanying drawings, wherein like numbers reference like elements.

[0022] FIG. **1** is an application example of an ultrasonic blood pressure measuring device.

[0023] FIG. **2** is an explanatory diagram of the measurement of a blood vessel diameter using an ultrasonic wave.

[0024] FIG. **3** is a graph showing the relationship between the blood vessel diameter and blood pressure.

[0025] FIG. **4**A is a graph of a blood vessel diameter variation waveform, and FIG. **4**B is a graph of a displacement acceleration waveform of the blood vessel wall.

[0026] FIG. **5** is a diagram showing the functional configuration of the ultrasonic blood pressure measuring device.

[0027] FIG. **6** is a flowchart of the blood pressure measuring process.

[0028] FIG. **7**A is a graph of a blood vessel diameter variation waveform, and FIG. **7**B is a graph of a displacement speed waveform of the blood vessel wall.

[0029] FIG. **8** is a diagram showing a modification example of correlation setting data.

DESCRIPTION OF EXEMPLARY EMBODIMENTS

Overall Configuration

[0030] FIG. **1** is a diagram showing an application example of an ultrasonic blood pressure measuring device **10** in the present embodiment. The ultrasonic blood pressure measuring device **10** is a device that measures the blood pressure of a subject **2** in a non-pressure manner using an ultrasonic wave, and includes a main body **20** and an ultrasonic probe **30**.

[0031] The ultrasonic probe **30** has an ultrasonic transducer **32** (refer to FIG. **2**) to transmit and receive an ultrasonic pulse signal or burst signal of, for example, several to tens of MHz, and outputs a received signal to the main body **20**. The ultrasonic probe **30** is attached to the neck skin surface of the subject **2** so that the ultrasonic transducer **32** is located immediately above the carotid artery of the subject **2**, for example. Here, "immediately above" is used as an operating manual expression when operating the ultrasonic probe **30** for easy understanding. To be precise, "immediately above" refers to the positional relationship when the carotid artery is located on the straight line of irradiation of the ultrasonic wave emitted from the ultrasonic transducer **32**.

[0032] The main body **20** is connected to the ultrasonic probe **30** by a cable, and measures the blood pressure of the subject **2** using the ultrasonic probe **30**. Specifically, the main body **20** emits an ultrasonic wave toward the blood vessel (for example, carotid artery) of the subject **2** using the ultrasonic probe **30**, measures the position of the blood vessel wall and a blood vessel diameter based on the received signal of the reflected wave, and calculates the blood pressure of the subject **2** based on the measured position of the blood vessel wall and the measured blood vessel diameter. In particular, the present embodiment is characterized in that cardiac systolic blood pressure (highest blood pressure) and cardiac diastolic blood pressure (lowest blood pressure) are measured and output for each heartbeat. In general, terms of systolic blood pressure and diastolic blood pressure are used. In the present embodiment, however, contraction and expansion of the blood vessel are also handled. Therefore, in order to avoid confusion, terms of cardiac systolic blood pressure and cardiac diastolic blood pressure are used.

[0033] In addition, in calculating the blood pressure based on the blood vessel diameter, it is necessary to measure the blood pressure for calibration apart from the blood vessel diameter. For this blood pressure measurement, it is assumed that a pressure sphygmomanometer **40** is used in the present embodiment. The pressure sphygmomanometer **40** measures the blood pressure of the arm artery of the subject **2** in a state where a cuff for pressure **42** is wound around the upper arm of the subject **2**. After calibration, the cuff **42** is detached from the subject **2**. Then, the blood pressure of the subject **2** is measured in a non-pressure manner, that is, in a non-invasive manner using the ultrasonic probe **30**.

Principle

(1) Measurement of Position of Blood Vessel Wall and Blood Vessel Diameter

[0034] First, measurement of the position of a blood vessel wall and a blood vessel diameter using an ultrasonic wave will be described. The blood vessel diameter can be calculated from the position of the blood vessel wall, more specifically, from the depth positions (hereinafter, simply referred to as "positions") of the front and rear walls of the blood vessel. Therefore, if the depth positions of the front and rear walls of the blood vessel are measured, the blood vessel diameter can be automatically calculated. FIG. **2** is a diagram for explaining the measurement of the position of a blood vessel wall and a blood vessel diameter using an ultrasonic wave, and shows a cross-sectional view of a blood vessel **4** in a long-axis direction thereof. As shown in FIG. **2**, in measurement, the ultrasonic probe **30** is attached to the neck of the subject **2** so that the ultrasonic transducer **32** is in close contact with a skin surface **3** immediately above the blood vessel **4**.

[0035] From the ultrasonic transducer **32**, an ultrasonic wave is transmitted in a downward direction in FIG. **2**. The ultrasonic wave has a characteristic of being largely reflected on the boundary surface of the medium. That is, when the blood vessel **4** is located immediately below the ultrasonic transducer **32**, some of the ultrasonic waves transmitted from the ultrasonic transducer **32** are reflected on a front wall **4***a* and a rear wall **4***b* of the blood vessel **4**, and strong reflected waves reflected from the front wall **4***a* and the rear wall **4***b* appear in the reflected wave signal in the ultrasonic transducer **32**. The positions of the front wall **4***a* and the rear wall **4***b* can be measured from the time difference until reflected waves from the front wall **4***a* and the rear wall **4***b* appear from the ultrasonic wave transmission timing and the propagation speed of the ultrasonic wave. A blood vessel diameter D is calculated by finding the positions of the front wall **4***a* and the rear wall **4***b*. The measurement of the position of the blood vessel wall and the blood vessel diameter using an ultrasonic wave is repeatedly performed at predetermined periods of several to tens of milliseconds, for example. The measurement unit is referred to as a "frame" hereinafter.

(2) Correlation Between Blood Vessel Diameter and Blood Pressure

[0036] Next, measurement of blood pressure based on the blood vessel diameter will be described. FIG. **3** is a graph showing the correspondence relationship between the blood vessel diameter D and blood pressure P. As shown in FIG. **3**, correlation between the blood vessel diameter D and the blood pressure P is a non-linear relationship, and it is known that the correlation between the blood vessel diameter D and the blood pressure P can be expressed by the correlation equation shown in the following equation (1).

$$P=Pd\cdot\exp[\beta(D/Dd-1)] \quad (1)$$

$$\text{Here, } \beta=\ln(Ps/Pd)/(Ds/Dd-1) \quad (2)$$

[0037] In the equations (1) and (2), "Pd" is a cardiac diastolic blood pressure (lowest blood pressure), "Dd" is a cardiac diastolic blood vessel diameter that is a blood vessel diameter at the time of cardiac diastolic blood pressure, "Ps" is a cardiac systolic blood pressure (highest blood pressure), "Ds" is a cardiac systolic blood vessel diameter that is a blood vessel diameter at the time of cardiac systolic blood pressure, and "β" is a blood vessel elasticity index value called a stiffness parameter.

[0038] In order to calculate the blood pressure P from the blood vessel diameter D using the correlation equation (1), it is necessary to set the cardiac diastolic blood pressure Pd, the cardiac diastolic blood vessel diameter Dd, the cardiac systolic blood pressure Ps, the cardiac systolic blood vessel diameter Ds, and the stiffness parameter β that are constants of the equations (1) and (2) and to perform a calibration to define the correlation equation (1). Therefore, in the present embodiment, the cardiac diastolic blood vessel diameter Dd and the cardiac systolic blood vessel diameter Ds are measured using the ultrasonic probe **30** and the cardiac diastolic blood pressure Pd and the cardiac systolic blood pressure Ps are measured using the pressure sphygmomanometer **40**, and the stiffness parameter β is calculated by using the measurement values Dd, Ds, Pd, and Ps, thereby defining the correlation equation (1). In addition, the cardiac diastolic blood pressure Pd and the cardiac systolic blood pressure Ps for calibration do not need to be measured by the pressure sphygmomanometer **40**, and may be measured by different measuring means.

[0039] After calibration, based on the measured blood vessel diameter D, it is possible to estimate the blood pressure P from the correlation equation (1). That is, in the present embodiment, a cardiac systolic blood vessel diameter Ds**1** and a cardiac diastolic blood vessel diameter Dd**1** are measured by ultrasonic measurement, and cardiac systolic blood pressure Ps**1** and cardiac diastolic blood pressure Pd**1** are calculated from the correlation equation (1) based on the cardiac systolic blood vessel diameter Ds**1** and the cardiac diastolic blood vessel diameter Dd**1** that have been measured.

(3) Measurement of Cardiac Systolic Blood Vessel Diameter Ds1 and Cardiac Diastolic Blood Vessel Diameter Dd1

[0040] Next, measurement of the cardiac systolic blood vessel diameter Ds**1** and the cardiac diastolic blood vessel diameter Dd**1** using an ultrasonic wave will be described. A blood vessel repeats contraction and expansion approximately isotropically due to the beating of the heart. That is, the blood vessel diameter varies approximately similar to blood pressure.

[0041] FIG. **4**A is a blood vessel diameter change waveform showing a temporal change in the blood vessel diameter of the carotid artery in one heartbeat period. In FIG. **4**A, the horizontal axis indicates time t, and the vertical axis indicates the blood vessel diameter D. One heartbeat period includes diastole and systole. That is, the blood vessel diameter increases and accordingly the carotid artery vessel expands rapidly from cardiac systole according to the beating of the heart. In cardiac diastole, the blood vessel diameter decreases slowly to return to the original thickness. Thus, since the blood vessel diameter increases rapidly in cardiac systole, a blood vessel diameter variation waveform rises rapidly. However, since the blood vessel diameter decreases slowly in cardiac diastole, the blood vessel diameter variation waveform falls slowly. In the blood vessel diameter variation waveform, the minimum value of the blood vessel diameter is a cardiac diastolic blood vessel diameter Dd**1**, and the maximum value of the blood vessel diameter is a cardiac systolic blood vessel diameter Ds**1**. In the present embodiment, the cardiac systolic blood vessel diameter Ds**1** and the cardiac diastolic blood vessel diameter Dd**1** are acquired by using the degree of displacement of the blood vessel wall.

[0042] FIG. **4**B is a waveform showing the displacement acceleration of the front wall of the blood vessel wall. In FIG. **4**B, the horizontal axis indicates time t that is used in common with FIG. **4**A, and the vertical axis indicates displacement acceleration. In the vertical direction, an upward direction is a direction in which the depth position becomes shallow, and a downward direction is a direction in which the depth position becomes deep. The displacement acceleration is an example of the degree of displacement of the blood vessel wall. For example, the displacement acceleration is obtained by differentiating the depth position of the blood vessel wall between a plurality of consecutive frames twice in a time direction based on the frame rate. In the following explanation, a blood vessel wall for which displacement acceleration is to be measured is a front wall of the blood vessel facing the skin side. However, the blood vessel wall for which displacement acceleration is to be measured may be a rear wall. In this case, the waveform shown in FIG. **4**B is vertically inverted.

[0043] A carotid artery vessel expands rapidly in cardiac systole, and returns to the original thickness slowly in cardiac diastole. That is, the depth position of the front wall of the carotid artery vessel changes in a direction in which the depth position of the front wall becomes shallow rapidly in cardiac systole and then changes in a direction in which the depth position of the front wall becomes deep slowly in cardiac diastole. Therefore, in the displacement acceleration waveform of the front wall of the blood vessel wall, the positive peak (maximum value) M**1** and the negative peak (minimum value) M**2** appear in order in the cardiac systole. Also in the cardiac diastole, a positive peak (maximum value) and a negative peak (minimum value) appear. However, since a change in the blood vessel diameter is gentle compared with that in the cardiac systole, the value of the peak is small.

[0044] That is, the cardiac systolic blood vessel diameter Ds**1** and the cardiac diastolic blood vessel diameter Dd**1** appear before and after the peak M**1** in cardiac systole of the displacement acceleration waveform of the blood vessel wall. Specifically, the peak M**1** indicates a peak of the blood vessel diameter, the cardiac systolic blood vessel diameter Ds**1** appears as a maximum value of the blood vessel diameter immediately after the peak M**1**, and the cardiac diastolic blood vessel diameter Dd**1** appears as a minimum value of blood vessel diameter immediately before the peak M**1**.

[0045] Therefore, a predetermined period Tw including the peak M**1** of the displacement acceleration waveform of the blood vessel wall is set, and the maximum value of the blood vessel diameter D in the predetermined period Tw is detected as the cardiac systolic blood vessel diameter Ds**1** and the minimum value of the blood vessel diameter D is detected as the cardiac diastolic blood vessel diameter Dd**1**. The predetermined period Tw is set so as to include the maximum value (cardiac systolic blood vessel diameter Ds**1**) and the minimum value (cardiac diastolic blood vessel diameter Dd**1**) of the blood vessel diameter variation waveform. Specifically, the predetermined period Tw is set as a period that is longer than the length of cardiac systole and is shorter than one heartbeat period, and can be set to about hundreds of milliseconds, for example, "about 100 to 300 milliseconds".

[0046] In addition, the peak M**1** in the displacement acceleration waveform of the blood vessel wall is detected by the displacement acceleration exceeding the predetermined threshold value A, and a time at which the peak M**1** is detected is determined to be the peak. The predetermined threshold value A is set to a value that is smaller than the peak M**1** of cardiac systole in the displacement acceleration waveform and is larger than the peak that may appear in cardiac diastole. In addition, the displacement acceleration waveform of the blood vessel wall differs depending on the subject **2**. Therefore, for example, it is also possible to acquire a displacement acceleration waveform from the waveform of the depth position of the blood vessel wall acquired in advance at the time of calibration or the like and to set the threshold value A according to the magnitude of the positive peak in the displacement acceleration waveform.

[0047] The cardiac systolic blood vessel diameter Ds**1** and the cardiac diastolic blood vessel diameter Dd**1** are calculated after the predetermined period Tw has ended. That is, after the predetermined period Tw has passed in ultrasonic measurement, the cardiac systolic blood vessel diameter Ds**1** that is the maximum value of the blood vessel diameter in the predetermined period Tw and the cardiac diastolic blood vessel diameter Dd**1** that is the minimum value of the blood vessel diameter are calculated, and the cardiac systolic blood pressure Ps**1** and the cardiac diastolic blood pressure Pd**1** are calculated from equation (1), thereby calculating the blood pressure. The time required for this processing is "about 100 to 200 milliseconds" at most. Accordingly, for each heartbeat, the cardiac systolic blood pressure Ps**1** and the cardiac diastolic blood pressure Pd**1** in the heartbeat can be immediately calculated and output before the next heartbeat arrives. As a result, it is possible to realize quick and continuous measurement.

Functional Configuration

[0048] FIG. **5** is a diagram showing the functional configuration of the ultrasonic blood pressure measuring device **10**. As shown in FIG. **5**, the ultrasonic blood pressure measuring device **10** is configured to include the ultrasonic probe **30** and the main body **20**. The main body **20** is configured to include an operation unit **110**, a display unit **120**, a sound output unit **130**, a communication unit **140**, a processing unit **200**, and a storage unit **300**.

[0049] The operation unit **110** is implemented by input devices, such as button switches, a touch panel, and various sensors, and outputs an operation signal corresponding to the operation to the processing unit **200**. The display unit **120** is implemented by a display device, such as a liquid crystal display (LCD), and performs various kinds of display according to the display signal from the processing unit **200**. The sound output unit **130** is implemented by a sound output device, such as a speaker, and outputs various sounds based on the sound signal from the processing unit **200**. The communication unit **140** is implemented by a wireless communication device, such as a wireless local area network (LAN) or Bluetooth (registered trademark), and performs communication with an external device (mainly, the pressure sphygmomanometer **40**).

[0050] The processing unit **200** is implemented by a microprocessor, such as a central processing unit (CPU) or a digital signal processor (DSP), or an electronic component, such as an application specific integrated circuit (ASIC) or an integrated circuit (IC) memory. The processing unit **200** controls the operation of the ultrasonic blood pressure measuring device **10** by executing various kinds of arithmetic processing based on a program or data stored in the storage unit **300**, an operation signal from the operation unit **110**, or the like. In addition, the processing unit **200** includes an ultrasonic measurement control section **210**, a blood vessel wall position and blood vessel diameter calculation section **220**, a correlation setting section **230**, a displacement degree measuring section **240**, a blood vessel diameter feature value acquisition section **250**, and a blood pressure calculation section **260**, and executes blood pressure measurement processing (refer to FIG. **6**) according to a blood pressure measurement program **310**.

[0051] The ultrasonic measurement control section **210** controls the transmission and reception of an ultrasonic wave in the ultrasonic probe **30**. Specifically, the ultrasonic measurement control section **210** transmits an ultrasonic wave from the ultrasonic probe **30** at the transmission timing of a predetermined period. In addition, the ultrasonic measurement control section **210** performs amplification or the like of the signal of the reflected wave of the ultrasonic wave received by the ultrasonic probe **30**. Based on the received signal of the reflected wave by the ultrasonic probe **30**, ultrasonic measurement data **320** of each mode, such as an A mode, a B mode, or an M mode, is generated.

[0052] The blood vessel wall position and blood vessel diameter calculation section **220** calculates the position of the blood vessel wall and the blood vessel diameter based on the received signal of the reflected wave of the ultrasonic wave received by the ultrasonic probe **30**. That is, the reception of the reflected wave from each of the front wall **4***a* and the rear wall **4***b* of the blood vessel **4** is determined from the signal strength of the received signal. The positions (depth positions) of the front wall **4***a* and the rear wall **4***b* are calculated using the time difference between the ultrasonic wave transmission timing and the reception timing of the reflected waves from the front wall **4***a* and the rear wall **4***b*. Then, the blood vessel diameter is calculated from the positions of the front wall **4***a* and the rear wall **4***b*. Since the transmission of the ultrasonic wave and the reception of the reflected wave by the ultrasonic probe **30** are performed when necessary, the calculation of the position of the blood vessel wall and the blood vessel diameter is repeatedly executed at every predetermined time (for example, at time intervals that can be called almost real time, such as several to tens of milliseconds). As a result, a waveform (refer to FIG. **4**A) showing the variation of the blood vessel diameter is obtained. The blood vessel diameter obtained by the blood vessel wall position and blood vessel diameter calculation section **220** is stored as blood vessel diameter measurement data **350** so as to match the measurement time.

[0053] The correlation setting section **230** sets the correlation between the blood vessel diameter D and the blood pressure P based on the calculation result of the blood vessel wall position and blood vessel diameter calculation section **220** and the measurement result of the pressure sphygmomanometer **40**. That is, the correlation equation (1) indicating the correlation between the blood vessel diameter and blood pressure is set and defined by calculating the stiffness parameter β given by equation (2) from the cardiac systolic blood pressure Ps, the cardiac diastolic blood pressure Pd, the cardiac systolic blood vessel diameter Ds, and the cardiac diastolic blood vessel diameter Dd. The correlation setting section **230** can also be said to be a calibration section that calibrates the correlation between the blood vessel diameter and blood pressure.

[0054] The cardiac systolic blood pressure Ps and the cardiac diastolic blood pressure Pd are measured by the pressure sphygmomanometer **40**. Blood pressure measurement using the pressure sphygmomanometer **40** takes a time of about several to tens of seconds. The cardiac systolic blood vessel diameter Ds and the cardiac diastolic blood vessel diameter Dd are calculated from the blood vessel diameter calculated by the blood vessel wall position and blood vessel diameter calculation section **220**, the calculation by the blood vessel diameter calculation section **220** being performed in parallel with the blood pressure measurement using the pressure sphygmomanometer **40**. That is, the maximum value and the minimum value of the blood vessel diameter are detected for each heartbeat, and the maximum values is set to the cardiac systolic blood vessel diameter Ds and the minimum values is set to the cardiac diastolic blood vessel diameter Dd.

[0055] The blood pressure measured by the pressure sphygmomanometer **40** is stored as blood pressure measurement data **340** so as to match the measurement. In addition, the correlation between the blood vessel diameter and blood pressure set by the correlation setting section **230** is stored as correlation setting data **330**. Specifically, the correlation setting data **330** stores the values of the parameter Ds, Dd, Ps, Pd, and β defining the correlation equation (1).

[0056] The displacement degree measuring section **240** measures the displacement acceleration of the front wall of the blood vessel that is the degree of displacement of the blood vessel wall. That is, displacement acceleration is calculated from a temporal change in the position of the front wall **4***a* of the blood vessel calculated by the blood vessel wall position and blood vessel diameter calculation section **220**.

[0057] The blood vessel diameter feature value acquisition section **250** calculates the cardiac systolic blood vessel diameter Ds**1** and the cardiac diastolic blood vessel diameter Dd**1**, which are feature values of the blood vessel diameter, from the blood vessel diameter calculated by the blood vessel wall position and blood vessel diameter calculation section **220**. That is, the blood vessel diameter feature value acquisition section **250** regards displacement acceleration when the displacement acceleration of the blood vessel wall measured by the displacement degree measuring section **240** exceeds a predetermined threshold value as the peak M**1** (value of the peak: maximum value), and sets the predetermined period Tw with the time of the peak M**1** as a reference. Then, the maximum value and the minimum value of the blood vessel diameter in the set predetermined period Tw are determined, and the determined maximum value is set to the cardiac systolic blood vessel diameter Ds**1** and the minimum value is set to the cardiac diastolic blood vessel diameter Dd**1**. The blood vessel diameter feature value acquisition section **250** corresponds to a peak calculation section and a blood vessel diameter acquisition section. The feature values (cardiac systolic blood vessel diameter Ds**1** and cardiac diastolic blood vessel diameter Dd**1**) of the blood vessel diameter calculated by the blood vessel diameter feature value acquisition section **250** are stored as blood vessel diameter feature value data **360**.

[0058] The blood pressure calculation section **260** calculates the cardiac systolic blood pressure Ps**1** and the cardiac diastolic blood pressure Pd**1**, according to the correlation equation (1) set by the correlation setting section **230**, based on the cardiac systolic blood vessel diameter Ds**1** and the cardiac diastolic blood vessel diameter Dd**1** that are feature values of the blood vessel diameter calculated by the blood vessel diameter feature value acquisition section **250**. The systolic blood pressure Ps**1** and the cardiac diastolic blood pressure Pd**1** calculated by the blood pressure calculation section **260** are stored as blood pressure calculation data **370** so as to match the measurement time.

[0059] The storage unit **300** is implemented by a storage device, such as a read only memory (ROM), a random access memory (RAM), or a hard disk. The storage unit **300** stores a program or data required for the processing unit **200** to perform overall control of the ultrasonic blood pressure measuring device **10**, and is used as a working area of the processing unit **200**. In addition, the calculation results of the processing unit **200**, operation data from the operation unit **110**, and the like are temporarily stored in the storage unit **300**. n the present embodiment, the blood pressure measurement program **310**, the ultrasonic measurement data **320**, the correlation setting data **330**, the blood pressure measurement data **340**, the blood vessel diameter measurement data **350**, the blood vessel diameter feature value data **360**, and the blood pressure calculation data **370** are stored in the storage unit **300**.

Process Flow

[0060] FIG. **6** is a flowchart illustrating the flow of the blood pressure measuring process. This process is realized by the processing unit **200** that executes the blood pressure measurement program **310**.

[0061] Referring to FIG. **6**, first, the measurement of the position of a blood vessel wall and a blood vessel diameter using an ultrasonic wave is started when the ultrasonic measurement control section **210** starts control to transmit and receive an ultrasonic wave to and from the ultrasonic probe **30** and the blood vessel wall position and blood vessel diameter calculation section **220** starts the measurement of the position of the blood vessel wall and the blood vessel diameter based on the received signal of the reflected wave of the ultrasonic wave (step S**1**).

[0062] Then, the processing unit **200** determines whether or not calibration is required. For example, the processing unit **200** determines that calibration is required when the subject **2** performs blood pressure measurement with the device for the first time or when a predetermined amount of time has passed from the previous calibration. If calibration is required (step S**3**: YES), for example, a message is displayed on the display unit **120** to give an instruction to attach the cuff **42** to the subject **2** and measure the blood pressure with the pressure sphygmomanometer **40**. Accordingly, blood pressure measurement of the subject **2** using the pressure sphygmomanometer **40** is started (step S**5**). When the blood pressure measurement using the pressure sphygmomanometer **40** ends and the highest blood pressure (cardiac systolic blood pressure) Ps and the lowest blood pressure (cardiac diastolic blood pressure) Pd are measured, the correlation setting section **230** calculates the stiffness parameter β from the blood vessel diameter obtained by ultrasonic measurement and the blood pressure measured by the pressure sphygmomanometer **40**, and calculates the correlation equation (1) between the blood vessel diameter and the blood pressure (step S**7**). This is the calibration.

[0063] After the calibration ends, the displacement degree measuring section **240** starts the calculation of the displacement acceleration of the blood vessel wall from the position of the blood vessel wall measured for each frame by the blood vessel wall position and blood vessel diameter calculation section **220** (step S**9**). Then, the blood vessel diameter feature value acquisition section **250** compares the calculated displacement acceleration with the predetermined threshold value A. If the displacement acceleration exceeds the predetermined threshold value A (step S**11**: YES), the blood vessel diameter feature value acquisition section **250** sets the predetermined period Tw including the time at which the displacement acceleration exceeds the predetermined threshold value A, and calculates the maximum value and the minimum value of the blood vessel diameter in the predetermined period Tw (step S**13**). Then, the maximum value is set to the cardiac systolic blood vessel diameter Ds**1**, and the minimum value is set to the cardiac diastolic blood vessel diameter Dd**1** (step S**15**).

[0064] Then, the blood pressure calculation section **260** calculates the cardiac systolic blood pressure Ps**1** and the cardiac diastolic blood pressure Pd**1** from the correlation equation (1) based on the cardiac systolic blood vessel diameter Ds**1** and the cardiac diastolic blood vessel diameter Dd**1** that have been calculated (step S**17**). Then, the cardiac systolic blood pressure Ps**1** and the cardiac diastolic blood pressure Pd**1** that have been calculated are displayed on the display unit **120**, and are stored as the blood pressure calculation data **370** (step S**19**).

[0065] Then, the processing unit **200** determines whether or not the blood pressure measurement using an ultrasonic wave has ended. If the blood pressure measurement has not ended (step S**21**: NO), the process returns to step S**11** to perform blood pressure measurement for the next heartbeat period. On the other hand, if the blood pressure measurement has ended (step S**21**: YES), the ultrasonic measurement control section **210** ends the transmission and reception of the ultrasonic wave by the ultrasonic probe **30**. After ending the measurement of the blood vessel diameter using an ultrasonic wave (step S**23**), this process is ended.

Effects

[0066] Thus, according to the ultrasonic blood pressure measuring device **10** of the present embodiment, the cardiac systolic blood pressure (highest blood pressure) and the cardiac diastolic blood pressure (lowest blood pressure) can be measured for each heartbeat. That is, the displacement acceleration of the position (depth position) of the blood vessel wall of the blood vessel measured by using an ultrasonic wave is calculated, the peak M**1** of the displacement acceleration is detected by comparing the displacement acceleration with the predetermined threshold value A, and the predetermined period Tw including the peak M**1** as a reference is set. Then, the minimum value of the blood vessel diameter in the predetermined period Tw is set to the cardiac diastolic blood vessel diameter Dd**1**, and the maximum value of the blood vessel diameter is set to the cardiac systolic blood vessel diameter Ds**1**. The cardiac systolic blood pressure Ps**1** and the cardiac diastolic blood pressure Pd**1** are calculated from the correlation equation (1) between the blood vessel diameter D and the blood pressure P. Therefore, since the cardiac systolic blood pressure and the cardiac diastolic blood pressure appearing for each heartbeat can be measured before the next heartbeat arrives, it is possible to measure the highest blood pressure (cardiac systolic blood pressure) and the lowest blood pressure (cardiac diastolic blood pressure) quickly and continuously.

Modification Examples

[0067] In addition, it should be understood that embodiments to which the invention can be applied are not limited to the embodiment described above and various modifications can be made without departing from the spirit and scope of the invention.

[0068] (A) In the embodiment described above, "displacement acceleration of the blood vessel wall" is used as the "degree of displacement of the blood vessel wall". However, "displacement speed of the blood vessel wall" may also be used.

[0069] FIG. **7**A is a blood vessel diameter variation waveform showing a temporal change in the blood vessel diameter of the carotid artery in one heartbeat period. FIG. **7**B is a waveform showing a displacement speed V that is an example of the degree of change of the blood vessel wall. The displacement speed waveform of the blood vessel wall is obtained by differentiating the position of the blood vessel wall between a plurality of consecutive frames once in a time direction based on the frame rate, for example. In FIG. **7**B, similar to the displacement acceleration shown in FIG. **4**B, the front wall of the blood vessel is an object to be measured, and the upward direction is a direction (positive direction) in which the position of the front wall becomes shallow.

[0070] As shown in FIG. **7**B, in the displacement speed of the blood vessel wall, a positive peak M**3** appears in cardiac systole. In addition, although the negative peak appears in cardiac diastole, the negative peak is a small peak value because the change in the blood vessel diameter is gentle compared with the cardiac systole. That is, the cardiac systolic blood vessel diameter Ds**1** and the cardiac diastolic blood vessel diameter Dd**1** appear before and after the peak M**3**. Specifically, the peak M**3** indicates a peak of the blood vessel diameter, the cardiac systolic blood vessel diameter Ds**1** appears as a maximum value of the blood vessel diameter immediately after the peak M**3**, and the cardiac diastolic blood vessel diameter Dd**1** appears as a minimum value of the blood vessel diameter immediately before the peak M**3**. Therefore, a predetermined period Tw including the peak M**3** of the displacement speed of the blood vessel wall as a reference can be set, and the maximum value of the blood vessel diameter D in the predetermined period Tw can be detected as the cardiac systolic blood vessel diameter Ds**1** and the minimum value of the blood vessel diameter D can be detected as the cardiac diastolic blood vessel diameter Dd**1**.

[0071] In addition, the peak M**3** in the displacement speed of the blood vessel wall is detected by the displacement speed exceeding a predetermined threshold value B, and a time at which the peak M**3** is detected is determined to be the peak. The predetermined threshold value B is set to a value that is smaller than the peak M**3** of cardiac systole.

[0072] (B) In the embodiment described above, the communication method of the ultrasonic blood pressure measuring device **10** and the pressure sphygmomanometer **40** is wired communication. However, wireless communication may also be applied. In addition, the subject **2** may be made to measure the blood pressure using, for example, the pressure sphygmomanometer **40**, and the subject **2** may manually input the measurement value to the ultrasonic blood pressure measuring device **10**.

[0073] (C) In the embodiment described above, the blood vessel to be measured is the carotid artery. However, it is needless to say that other arteries, such as the radial artery, can be applied as an object to be measured.

[0074] (D) In addition, in the embodiment described above, the correlation setting data **330** is data for storing the value of each parameter defining the correlation equation (1). However, other forms may also be applied. For example, after deriving the correlation equation (1) by calculating the value of each parameter, a look-up table shown in FIG. **8** in which the correspondence relationship between the blood vessel diameter and blood pressure is set may be obtained from the correlation equation (1), and the look-up table may be set as the correlation setting data **330**. A functional portion for obtaining the look-up table is a correlation setting section. The interval between blood vessel diameters in the look-up table can be arbitrarily set. For example, the interval between blood vessel diameters can be set to a unit of several to tens of micrometers.

[0075] In addition, the blood pressure calculation section **260** can calculate the cardiac systolic blood pressure Ps**1** and the cardiac diastolic blood pressure Pd**1** from the cardiac systolic blood vessel diameter Ds**1** and the cardiac diastolic blood vessel diameter Dd**1**, which have been calculated by the blood vessel diameter feature value acquisition section **250**, with reference to the look-up table. As a result, it is possible to reduce the calculation load when the blood pressure calculation section **260** calculates blood pressure.

[0076] The entire disclosure of Japanese Patent Application No. 2014-081925 filed on Apr. 11, 2014 and No. 2014-159626 filed on Aug. 5, 2014 are expressly incorporated by reference herein.

What is claimed is:

1. An ultrasonic blood pressure measuring device, comprising:

a transmission and reception unit that transmits an ultrasonic wave to a blood vessel and receives a reflected wave of the ultrasonic wave;

a displacement degree measuring unit that measures a degree of displacement of a blood vessel wall of the blood vessel based on reflected wave of the ultrasonic wave during at least one heartbeat period;

a blood vessel diameter measuring unit that measures a diameter of the blood vessel based on the reflected wave;

a peak calculation unit that calculates a peak of the degree of displacement of the blood vessel wall;

a blood vessel diameter acquisition unit that acquires a maximum value of the blood vessel diameter, which appears after the peak of the degree of displacement of the blood vessel wall, as a cardiac systolic blood vessel diameter and acquires a minimum value of the blood vessel diameter, which appears before the peak, as a cardiac diastolic blood vessel diameter; and

a blood pressure calculation unit that calculates cardiac systolic blood pressure and cardiac diastolic blood pressure from the cardiac systolic blood vessel diameter and the cardiac diastolic blood vessel diameter using a correlation between the diameter of the blood vessel and blood pressure set in advance.

2. The ultrasonic blood pressure measuring device according to claim **1**,

wherein the displacement degree measuring unit measures a displacement speed of the blood vessel wall as the degree of displacement.

3. The ultrasonic blood pressure measuring device according to claim **1**,

wherein the displacement degree measuring unit measures displacement acceleration of the blood vessel wall as the degree of displacement.

4. The ultrasonic blood pressure measuring device according to claim **1**, further comprising:

a correlation setting unit that sets the correlation.

5. The ultrasonic blood pressure measuring device according to claim **1**,

wherein the blood vessel is an artery.

6. The ultrasonic blood pressure measuring device according to claim **1**, further comprising:

a storage unit that stores the correlation as a look-up table of the blood vessel diameter and the blood pressure,

wherein the blood pressure calculation unit calculates cardiac systolic blood pressure and cardiac diastolic blood pressure from the cardiac systolic blood vessel diameter and the cardiac diastolic blood vessel diameter with reference to the look-up table.

7. An ultrasonic blood pressure measuring method, comprising:

receiving a reflected wave of an ultrasonic wave transmitted to a blood vessel and measuring a degree of displacement of a blood vessel wall of the blood vessel based on the reflected wave of the ultrasonic wave during at least one heartbeat period;

measuring a diameter of the blood vessel based on the reflected wave;

calculating a peak of the degree of displacement of the blood vessel wall; and

calculating cardiac systolic blood pressure and cardiac diastolic blood pressure from a maximum value of the blood vessel diameter, which appears after the peak of the degree of displacement of the blood vessel wall, and a minimum value of the blood vessel diameter, which appears before the peak, using a correlation between the diameter of the blood vessel and blood pressure set in advance.

* * * * *

patsnap

专利名称(译)	超声波血压测量装置和超声波血压测量方法		
公开(公告)号	US20150289835A1	公开(公告)日	2015-10-15
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[标]申请(专利权)人(译)	精工爱普生株式会社		
申请(专利权)人(译)	SEIKO EPSON CORPORATION		
当前申请(专利权)人(译)	SEIKO EPSON CORPORATION		
[标]发明人	MIZUKAMI HIROMITSU		
发明人	MIZUKAMI, HIROMITSU		
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摘要(译)

超声波血压测量装置接收传输到血管的超声波的反射波，并且在至少一个心跳周期期间基于超声波的反射波测量血管的血管壁的位移程度。 。然后，从血管壁的位移峰值之后出现的血管直径的最大值和血管直径的最小值计算心脏收缩血压和心脏舒张压。使用预先设定的血管直径和血压之间的相关性出现在峰值之前。