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**Al-Ali**

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(54) **PHYSIOLOGICAL TREND MONITOR**

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Feb. 12, 2008, now Pat. No. 7,880,606, which is a  
continuation of application No. 11/717,591, filed on  
Mar. 13, 2007, now Pat. No. 7,355,512, which is a  
continuation of application No. 11/405,815, filed on  
Apr. 18, 2006, now Pat. No. 7,190,261, which is a  
continuation of application No. 10/975,860, filed on  
Oct. 28, 2004, now Pat. No. 7,030,749, which is a  
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**G08B 29/00** (2006.01)

(52) **U.S. Cl.**  
USPC ..... **340/511**; 600/300; 600/323

(58) **Field of Classification Search**  
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600/323

See application file for complete search history.

(56) **References Cited**

**U.S. PATENT DOCUMENTS**

4,960,128 A	10/1990	Gordon et al.
4,964,408 A	10/1990	Hink et al.
5,041,187 A	8/1991	Hink et al.
5,069,213 A	12/1991	Polczynski
5,163,438 A	11/1992	Gordon et al.
5,319,355 A	6/1994	Russek
5,337,744 A	8/1994	Branigan
5,341,805 A	8/1994	Stavridi et al.
D353,195 S	12/1994	Savage et al.
D353,196 S	12/1994	Savage et al.
5,377,676 A	1/1995	Vari et al.
D359,546 S	6/1995	Savage et al.
5,431,170 A	7/1995	Mathews
D361,840 S	8/1995	Savage et al.
D362,063 S	9/1995	Savage et al.
5,452,717 A	9/1995	Branigan et al.
D363,120 S	10/1995	Savage et al.
5,456,252 A	10/1995	Vari et al.
5,479,934 A	1/1996	Imran
5,482,036 A	1/1996	Diab et al.
5,490,505 A	2/1996	Diab et al.
5,494,043 A	2/1996	O'Sullivan et al.

(Continued)

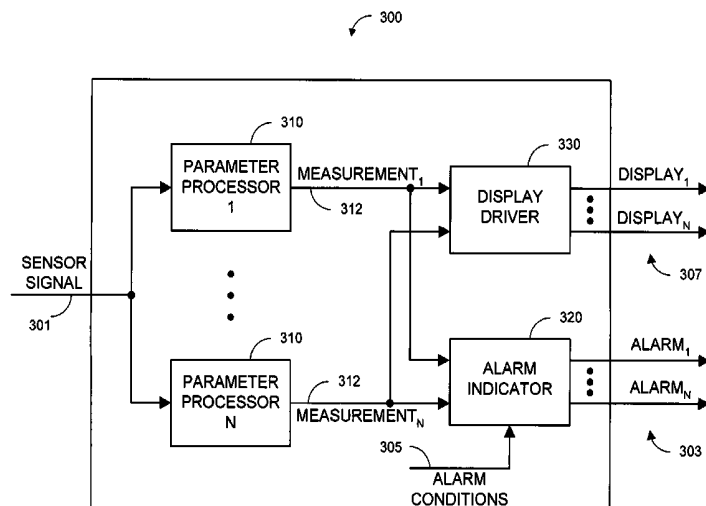
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Bear LLP

(57) **ABSTRACT**

A physiological trend monitor has a sensor signal responsive  
to multiple wavelengths of light transmitted into a tissue site.  
The transmitted light is detected after attenuation by pulsatile  
blood flow within the tissue site. A processor has an input  
responsive to the sensor signal and a physiological parameter  
output. Features are extracted from the physiological param-  
eter output. Criteria are applied to the features. An alarm  
output is generated when the criteria are satisfied.

**20 Claims, 9 Drawing Sheets**



(56)

## References Cited

## U.S. PATENT DOCUMENTS

5,533,511	A	7/1996	Kaspari et al.	6,463,311	B1	10/2002	Diab
5,534,851	A	7/1996	Russek	6,470,199	B1	10/2002	Kopotic et al.
5,561,275	A	10/1996	Savage et al.	6,501,975	B2	12/2002	Diab et al.
5,562,002	A	10/1996	Lalin	6,505,059	B1	1/2003	Kollias et al.
5,590,649	A	1/1997	Caro et al.	6,515,273	B2	2/2003	Al-Ali
5,602,924	A	2/1997	Durand et al.	6,519,487	B1	2/2003	Parker
5,632,272	A	5/1997	Diab et al.	6,525,386	B1	2/2003	Mills et al.
5,638,816	A	6/1997	Kiani-Azarbayjany et al.	6,526,300	B1	2/2003	Kiani et al.
5,638,818	A	6/1997	Diab et al.	6,541,756	B2	4/2003	Schulz et al.
5,645,440	A	7/1997	Tobler et al.	6,542,764	B1	4/2003	Al-Ali et al.
5,685,299	A	11/1997	Diab et al.	6,580,086	B1	6/2003	Schulz et al.
D393,830	S	4/1998	Tobler et al.	6,584,336	B1	6/2003	Ali et al.
5,743,262	A	4/1998	Lepper, Jr. et al.	6,595,316	B2	7/2003	Cybulski et al.
5,758,644	A	6/1998	Diab et al.	6,597,932	B2	7/2003	Tian et al.
5,760,910	A	6/1998	Lepper, Jr. et al.	6,597,933	B2	7/2003	Kiani et al.
5,769,785	A	6/1998	Diab et al.	6,606,511	B1	8/2003	Ali et al.
5,782,757	A	7/1998	Diab et al.	6,632,181	B2	10/2003	Flaherty et al.
5,785,659	A	7/1998	Caro et al.	6,639,668	B1	10/2003	Trepagnier
5,791,347	A	8/1998	Flaherty et al.	6,640,116	B2	10/2003	Diab
5,810,734	A	9/1998	Caro et al.	6,643,530	B2	11/2003	Diab et al.
5,823,950	A	10/1998	Diab et al.	6,650,917	B2	11/2003	Diab et al.
5,830,131	A	11/1998	Caro et al.	6,654,624	B2	11/2003	Diab et al.
5,833,618	A	11/1998	Caro et al.	6,658,276	B2	12/2003	Kianl et al.
5,860,919	A	1/1999	Kiani-Azarbayjany et al.	6,661,161	B1	12/2003	Lanzo et al.
5,890,929	A	4/1999	Mills et al.	6,671,531	B2	12/2003	Al-Ali et al.
5,904,654	A	5/1999	Wohltmann et al.	6,678,543	B2	1/2004	Diab et al.
5,919,134	A	7/1999	Diab	6,684,090	B2	1/2004	Ali et al.
5,934,925	A	8/1999	Tobler et al.	6,684,091	B2	1/2004	Parker
5,940,182	A	8/1999	Lepper, Jr. et al.	6,697,656	B1	2/2004	Al-Ali
5,995,855	A	11/1999	Kiani et al.	6,697,657	B1	2/2004	Shehada et al.
5,997,343	A	12/1999	Mills et al.	6,697,658	B2	2/2004	Al-Ali
6,002,952	A	12/1999	Diab et al.	RE38,476	E	3/2004	Diab et al.
6,011,986	A	1/2000	Diab et al.	6,699,194	B1	3/2004	Diab et al.
6,027,452	A	2/2000	Flaherty et al.	6,714,804	B2	3/2004	Al-Ali et al.
6,036,642	A	3/2000	Diab et al.	RE38,492	E	4/2004	Diab et al.
6,045,509	A	4/2000	Caro et al.	6,721,582	B2	4/2004	Trepagnier et al.
6,067,462	A	5/2000	Diab et al.	6,721,585	B1	4/2004	Parker
6,081,735	A	6/2000	Diab et al.	6,725,075	B2	4/2004	Al-Ali
6,088,607	A	7/2000	Diab et al.	6,728,560	B2	4/2004	Kollias et al.
6,110,522	A	8/2000	Lepper, Jr. et al.	6,735,459	B2	5/2004	Parker
6,124,597	A	9/2000	Shehada	6,745,060	B2	6/2004	Diab et al.
6,128,521	A	10/2000	Marro et al.	6,760,607	B2	7/2004	Al-Ali
6,129,675	A	10/2000	Jay	6,770,028	B1	8/2004	Ali et al.
6,144,868	A	11/2000	Parker	6,771,994	B2	8/2004	Kiani et al.
6,151,516	A	11/2000	Kiani-Azarbayjany et al.	6,792,300	B1	9/2004	Diab et al.
6,152,754	A	11/2000	Gerhardt et al.	6,813,511	B2	11/2004	Diab et al.
6,157,850	A	12/2000	Diab et al.	6,816,741	B2	11/2004	Diab
6,165,005	A	12/2000	Mills et al.	6,822,564	B2	11/2004	Al-Ali
6,184,521	B1	2/2001	Coffin, IV et al.	6,826,419	B2	11/2004	Diab et al.
6,206,830	B1	3/2001	Diab et al.	6,830,711	B2	12/2004	Mills et al.
6,229,856	B1	5/2001	Diab et al.	6,850,787	B2	2/2005	Weber et al.
6,232,609	B1	5/2001	Snyder et al.	6,850,788	B2	2/2005	Al-Ali
6,236,872	B1	5/2001	Diab et al.	6,852,083	B2	2/2005	Caro et al.
6,241,683	B1	6/2001	Macklem et al.	6,861,639	B2	3/2005	Al-Ali
6,253,097	B1	6/2001	Aronow et al.	6,898,452	B2	5/2005	Al-Ali et al.
6,256,523	B1	7/2001	Diab et al.	6,920,345	B2	7/2005	Al-Ali et al.
6,263,222	B1	7/2001	Diab et al.	6,931,268	B1	8/2005	Kiani-Azarbayjany et al.
6,278,522	B1	8/2001	Lepper, Jr. et al.	6,934,570	B2	8/2005	Kiani et al.
6,280,213	B1	8/2001	Tobler et al.	6,939,305	B2	9/2005	Flaherty et al.
6,285,896	B1	9/2001	Tobler et al.	6,943,348	B1	9/2005	Coffin, IV
6,301,493	B1	10/2001	Marro et al.	6,950,687	B2	9/2005	Al-Ali
6,317,627	B1	11/2001	Ennen et al.	6,961,598	B2	11/2005	Diab
6,321,100	B1	11/2001	Parker	6,970,792	B1	11/2005	Diab
6,325,761	B1	12/2001	Jay	6,979,812	B2	12/2005	Al-Ali
6,334,065	B1	12/2001	Al-Ali et al.	6,985,764	B2	1/2006	Mason et al.
6,343,224	B1	1/2002	Parker	6,993,371	B2	1/2006	Kiani et al.
6,349,228	B1	2/2002	Kiani et al.	6,996,427	B2	2/2006	Ali et al.
6,360,114	B1	3/2002	Diab et al.	6,999,904	B2	2/2006	Weber et al.
6,368,283	B1	4/2002	Xu et al.	7,003,338	B2	2/2006	Weber et al.
6,371,921	B1	4/2002	Caro et al.	7,003,339	B2	2/2006	Diab et al.
6,377,829	B1	4/2002	Al-Ali	7,015,451	B2	3/2006	Dalke et al.
6,388,240	B2	5/2002	Schulz et al.	7,024,233	B2	4/2006	Ali et al.
6,397,091	B2	5/2002	Diab et al.	7,027,849	B2	4/2006	Al-Ali
6,430,437	B1	8/2002	Marro	7,030,749	B2	4/2006	Al-Ali
6,430,525	B1	8/2002	Weber et al.	7,039,449	B2	5/2006	Al-Ali
				7,041,060	B2	5/2006	Flaherty et al.
				7,044,918	B2	5/2006	Diab
				7,067,893	B2	6/2006	Mills et al.
				7,096,052	B2	8/2006	Mason et al.

(56)

## References Cited

## U.S. PATENT DOCUMENTS

7,096,054	B2	8/2006	Abdul-Hafiz et al.	D606,659	S	12/2009	Kiani et al.
7,132,641	B2	11/2006	Schulz et al.	7,647,083	B2	1/2010	Al-Ali et al.
7,142,901	B2	11/2006	Kiani et al.	D609,193	S	2/2010	Al-Ali et al.
7,149,561	B2	12/2006	Diab	D614,305	S	4/2010	Al-Ali et al.
7,186,966	B2	3/2007	Al-Ali	RE41,317	E	5/2010	Parker
7,190,261	B2	3/2007	Al-Ali	7,729,733	B2	6/2010	Al-Ali et al.
7,215,984	B2	5/2007	Diab	7,734,320	B2	6/2010	Al-Ali
7,215,986	B2	5/2007	Diab	7,761,127	B2	7/2010	Al-Ali et al.
7,221,971	B2	5/2007	Diab	7,761,128	B2	7/2010	Al-Ali et al.
7,225,006	B2	5/2007	Al-Ali et al.	7,764,982	B2	7/2010	Dalke et al.
7,225,007	B2	5/2007	Al-Ali	D621,516	S	8/2010	Kiani et al.
RE39,672	E	6/2007	Shehada et al.	7,791,155	B2	9/2010	Diab
7,239,905	B2	7/2007	Kiani-Azarbayjany et al.	7,801,581	B2	9/2010	Diab
7,245,953	B1	7/2007	Parker	7,822,452	B2	10/2010	Schurman et al.
7,254,429	B2	8/2007	Schurman et al.	RE41,912	E	11/2010	Parker
7,254,431	B2	8/2007	Al-Ali	7,844,313	B2	11/2010	Kiani et al.
7,254,433	B2	8/2007	Diab et al.	7,844,314	B2	11/2010	Al-Ali
7,254,434	B2	8/2007	Schulz et al.	7,844,315	B2	11/2010	Al-Ali
7,272,425	B2	9/2007	Al-Ali	7,865,222	B2	1/2011	Weber et al.
7,274,955	B2	9/2007	Kiani et al.	7,873,497	B2	1/2011	Weber et al.
D554,263	S	10/2007	Al-Ali	7,880,606	B2	2/2011	Al-Ali
7,276,029	B2 *	10/2007	Goode et al. .... 600/300	7,880,626	B2	2/2011	Al-Ali et al.
7,280,858	B2	10/2007	Al-Ali et al.	7,891,355	B2	2/2011	Al-Ali et al.
7,289,835	B2	10/2007	Mansfield et al.	7,894,868	B2	2/2011	Al-Ali et al.
7,292,883	B2	11/2007	De Felice et al.	7,899,507	B2	3/2011	Al-Ali et al.
7,295,866	B2	11/2007	Al-Ali	7,899,518	B2	3/2011	Trepagnier et al.
7,328,053	B1	2/2008	Diab et al.	7,904,132	B2	3/2011	Weber et al.
7,332,784	B2	2/2008	Mills et al.	7,909,772	B2	3/2011	Popov et al.
7,340,287	B2	3/2008	Mason et al.	7,910,875	B2	3/2011	Al-Ali
7,341,559	B2	3/2008	Schulz et al.	7,919,713	B2	4/2011	Al-Ali et al.
7,343,186	B2	3/2008	Lamego et al.	7,937,128	B2	5/2011	Al-Ali
D566,282	S	4/2008	Al-Ali et al.	7,937,129	B2	5/2011	Mason et al.
7,355,512	B1	4/2008	Al-Ali	7,937,130	B2	5/2011	Diab et al.
7,356,365	B2	4/2008	Schurman	7,941,199	B2	5/2011	Kiani
7,371,981	B2	5/2008	Abdul-Hafiz	7,951,086	B2	5/2011	Flaherty et al.
7,373,193	B2	5/2008	Al-Ali et al.	7,957,780	B2	6/2011	Lamego et al.
7,373,194	B2	5/2008	Weber et al.	7,962,188	B2	6/2011	Kiani et al.
7,376,453	B1	5/2008	Diab et al.	7,962,190	B1	6/2011	Diab et al.
7,377,794	B2	5/2008	Al-Ali et al.	7,976,472	B2	7/2011	Kiani
7,377,899	B2	5/2008	Weber et al.	7,988,637	B2	8/2011	Diab
7,383,070	B2	6/2008	Diab et al.	7,990,382	B2	8/2011	Kiani
7,415,297	B2	8/2008	Al-Ali et al.	7,991,446	B2	8/2011	Ali et al.
7,428,432	B2	9/2008	Ali et al.	8,000,761	B2	8/2011	Al-Ali
7,438,683	B2	10/2008	Al-Ali et al.	8,008,088	B2	8/2011	Bellott et al.
7,440,787	B2	10/2008	Diab	RE42,753	E	9/2011	Kiani-Azarbayjany et al.
7,454,240	B2	11/2008	Diab et al.	8,019,400	B2	9/2011	Diab et al.
7,467,002	B2	12/2008	Weber et al.	8,028,701	B2	10/2011	Al-Ali et al.
7,469,157	B2	12/2008	Diab et al.	8,029,765	B2	10/2011	Bellott et al.
7,471,969	B2	12/2008	Diab et al.	8,036,728	B2	10/2011	Diab et al.
7,471,971	B2	12/2008	Diab et al.	8,046,040	B2	10/2011	Ali et al.
7,483,729	B2	1/2009	Al-Ali et al.	8,046,041	B2	10/2011	Diab et al.
7,483,730	B2	1/2009	Diab et al.	8,046,042	B2	10/2011	Diab et al.
7,489,958	B2	2/2009	Diab et al.	8,048,040	B2	11/2011	Kiani
7,496,391	B2	2/2009	Diab et al.	8,050,728	B2	11/2011	Al-Ali et al.
7,496,393	B2	2/2009	Diab et al.	RE43,169	E	2/2012	Parker
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7,499,741	B2	3/2009	Diab et al.	8,126,528	B2	2/2012	Diab et al.
7,499,835	B2	3/2009	Weber et al.	8,128,572	B2	3/2012	Diab et al.
7,500,950	B2	3/2009	Al-Ali et al.	8,130,105	B2	3/2012	Al-Ali et al.
7,509,154	B2	3/2009	Diab et al.	8,145,287	B2	3/2012	Diab et al.
7,509,494	B2	3/2009	Al-Ali	8,150,487	B2	4/2012	Diab et al.
7,510,849	B2	3/2009	Schurman et al.	8,175,672	B2	5/2012	Parker
7,526,328	B2	4/2009	Diab et al.	8,180,420	B2	5/2012	Diab et al.
7,530,942	B1	5/2009	Diab	8,182,443	B1	5/2012	Kiani
7,530,949	B2	5/2009	Al Ali et al.	8,185,180	B2	5/2012	Diab et al.
7,530,955	B2	5/2009	Diab et al.	8,190,223	B2	5/2012	Al-Ali et al.
7,532,919	B2 *	5/2009	Soyemi et al. .... 600/323	8,190,227	B2	5/2012	Diab et al.
7,563,110	B2	7/2009	Al-Ali et al.	8,203,438	B2	6/2012	Kiani et al.
7,596,398	B2	9/2009	Al-Ali et al.	8,224,411	B2	7/2012	Al-Ali et al.
7,618,375	B2	11/2009	Flaherty	8,228,181	B2	7/2012	Al-Ali
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\* cited by examiner

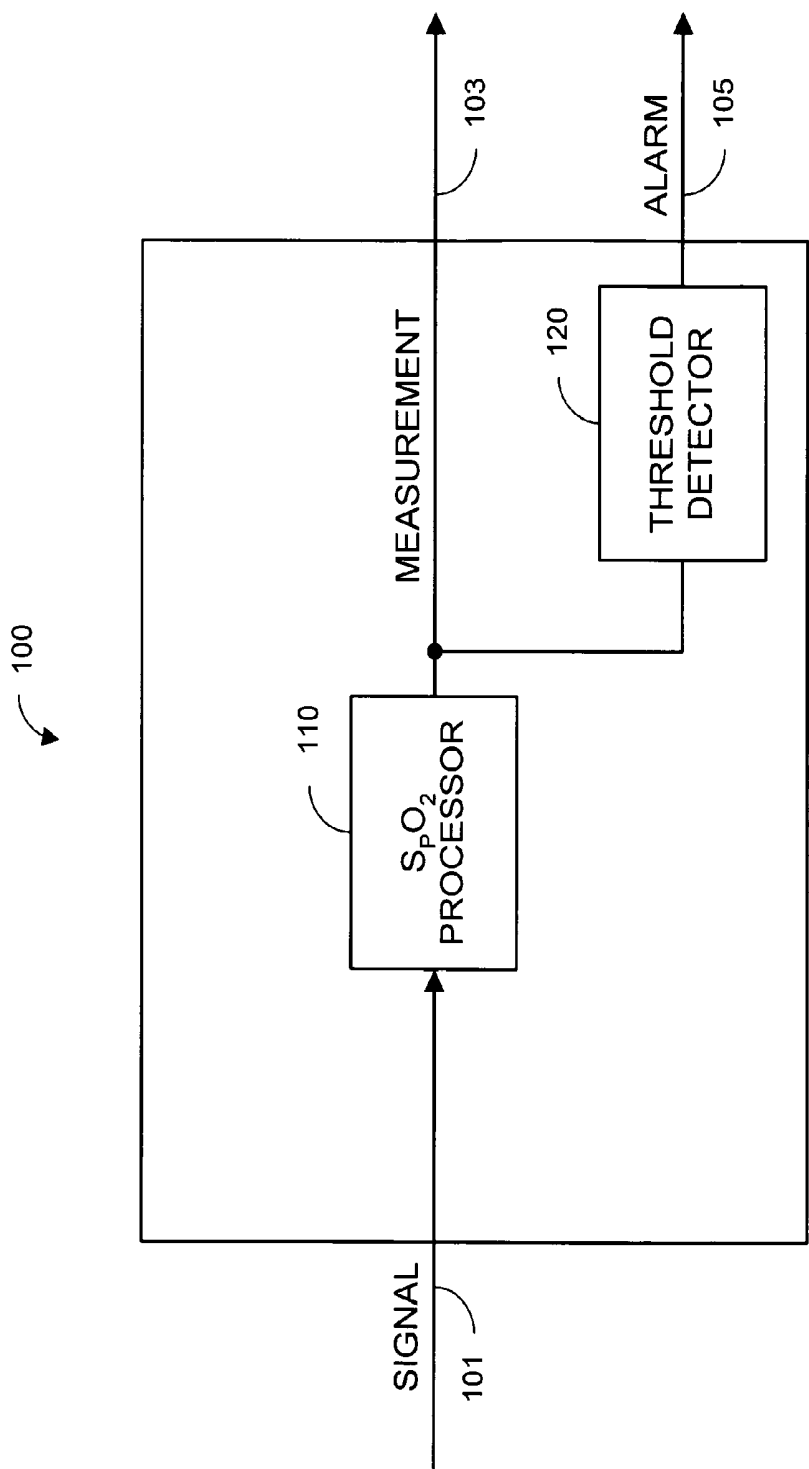


FIG. 1 (Prior Art)

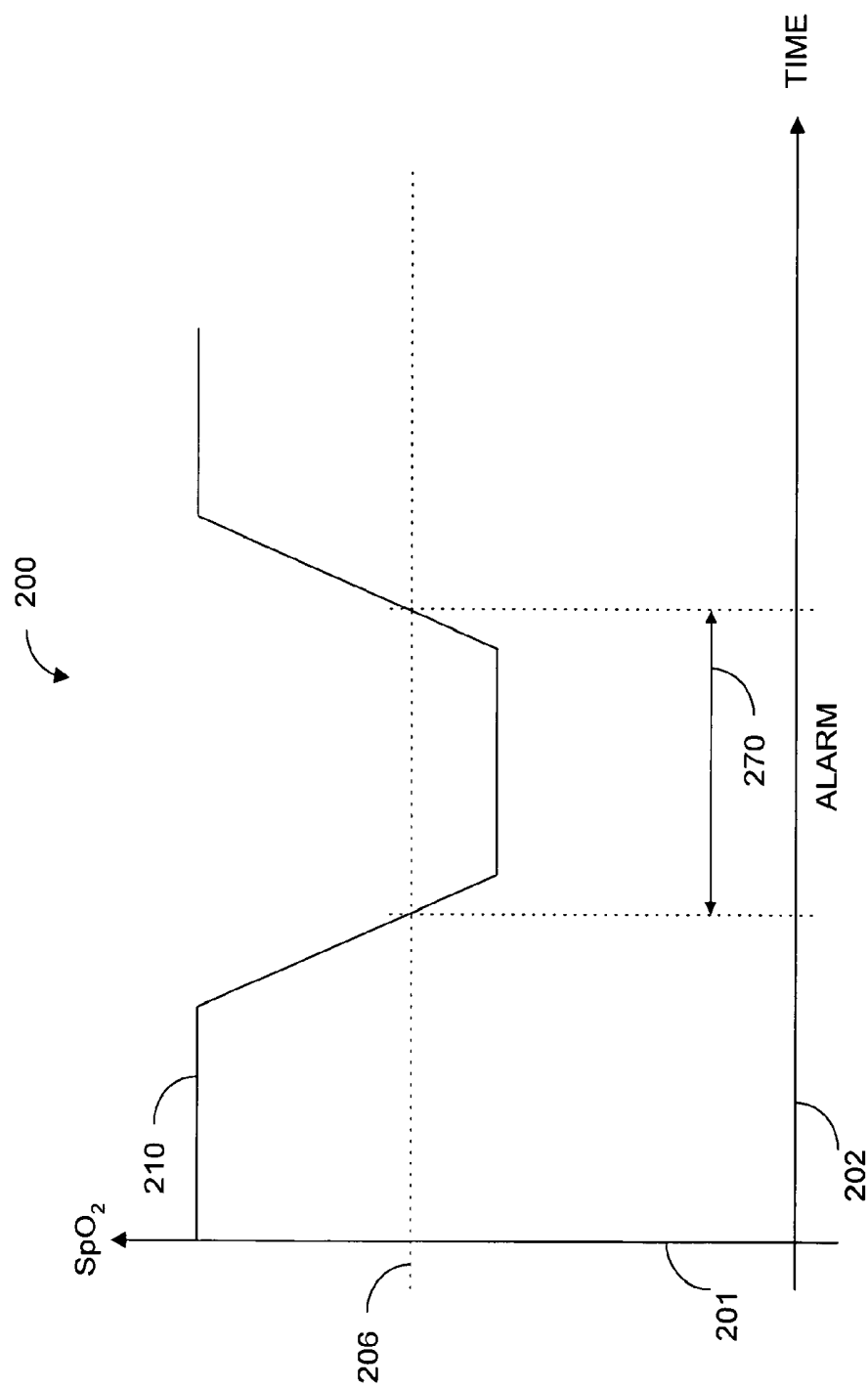


FIG. 2

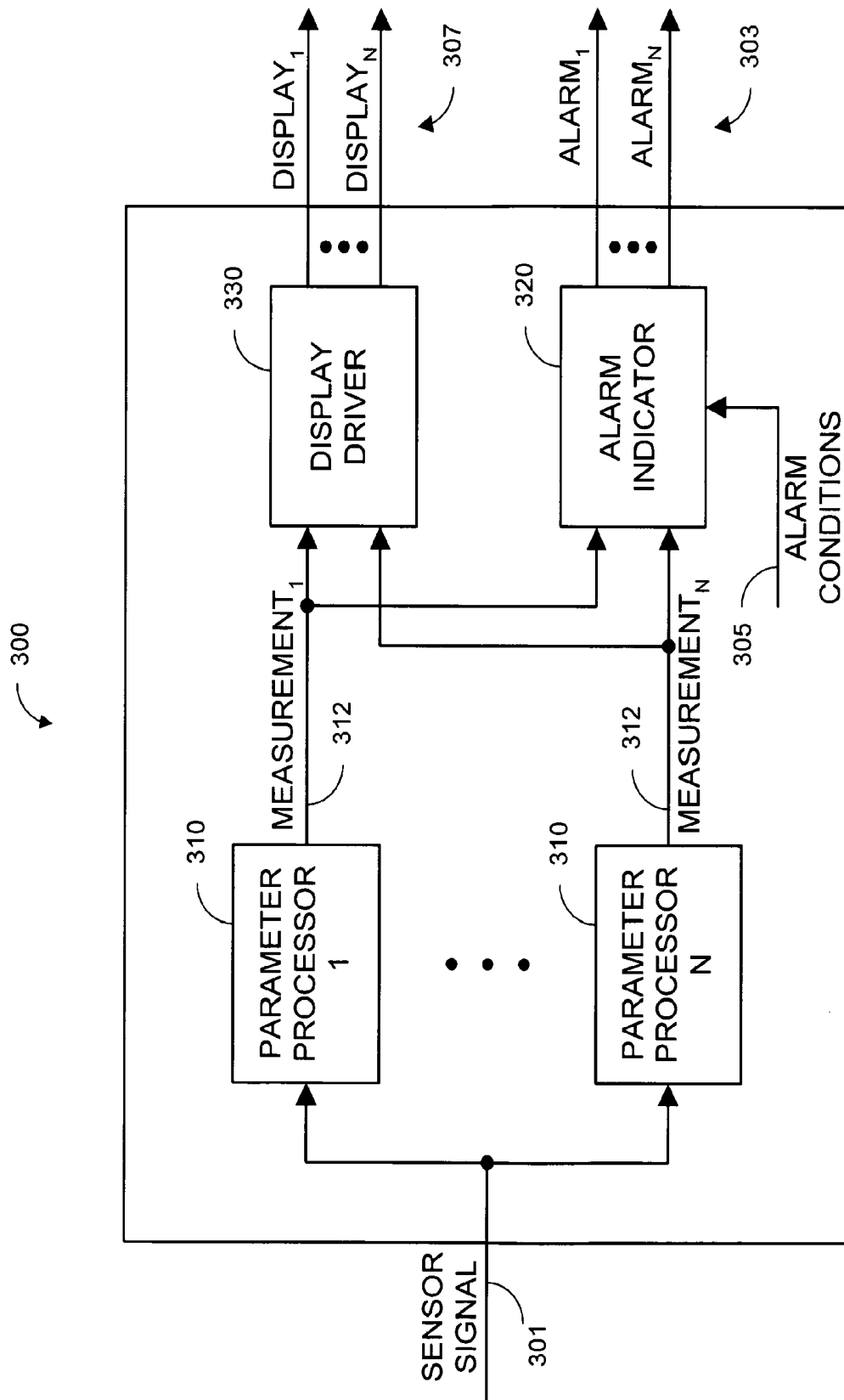


FIG. 3

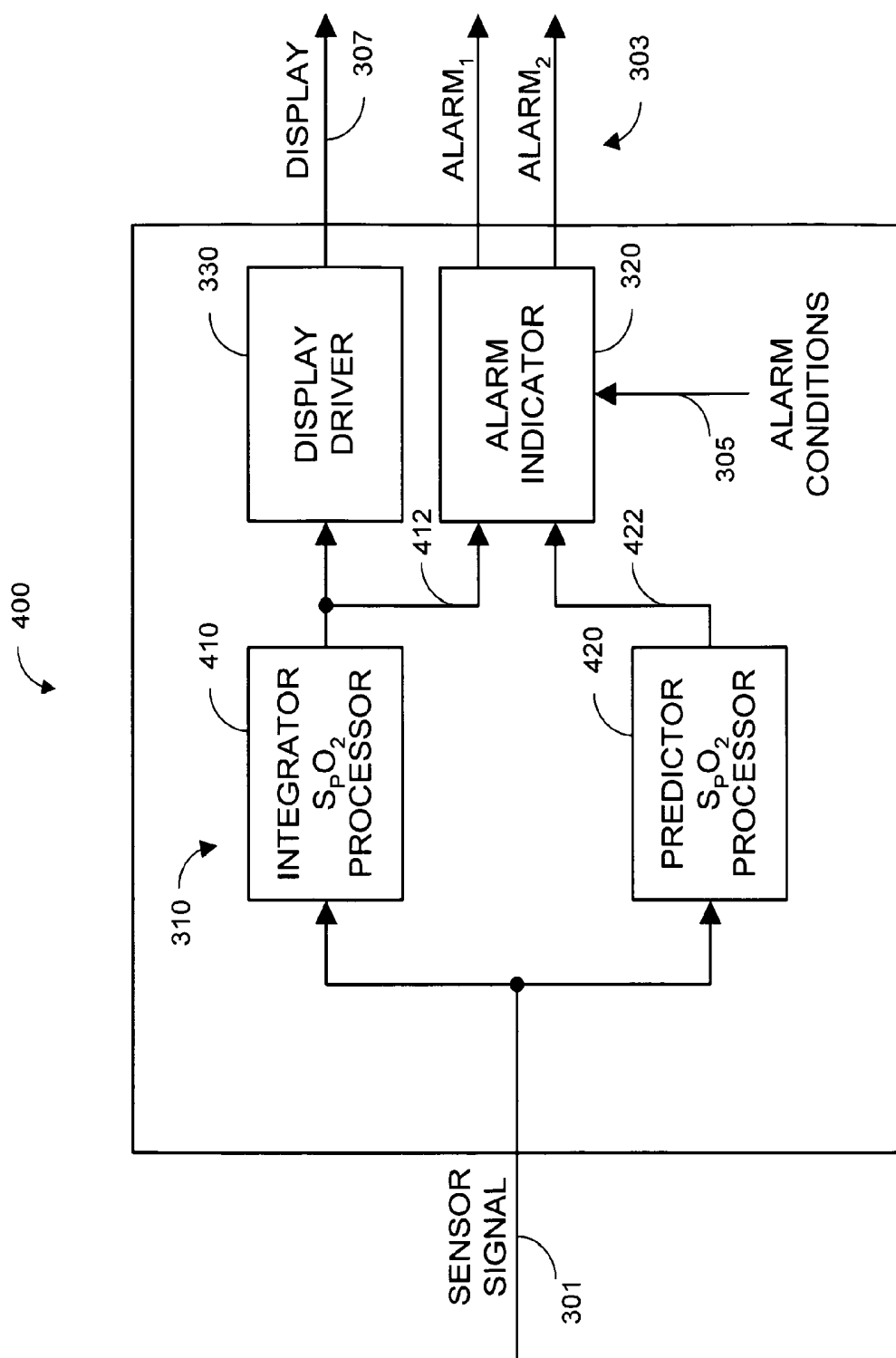


FIG. 4

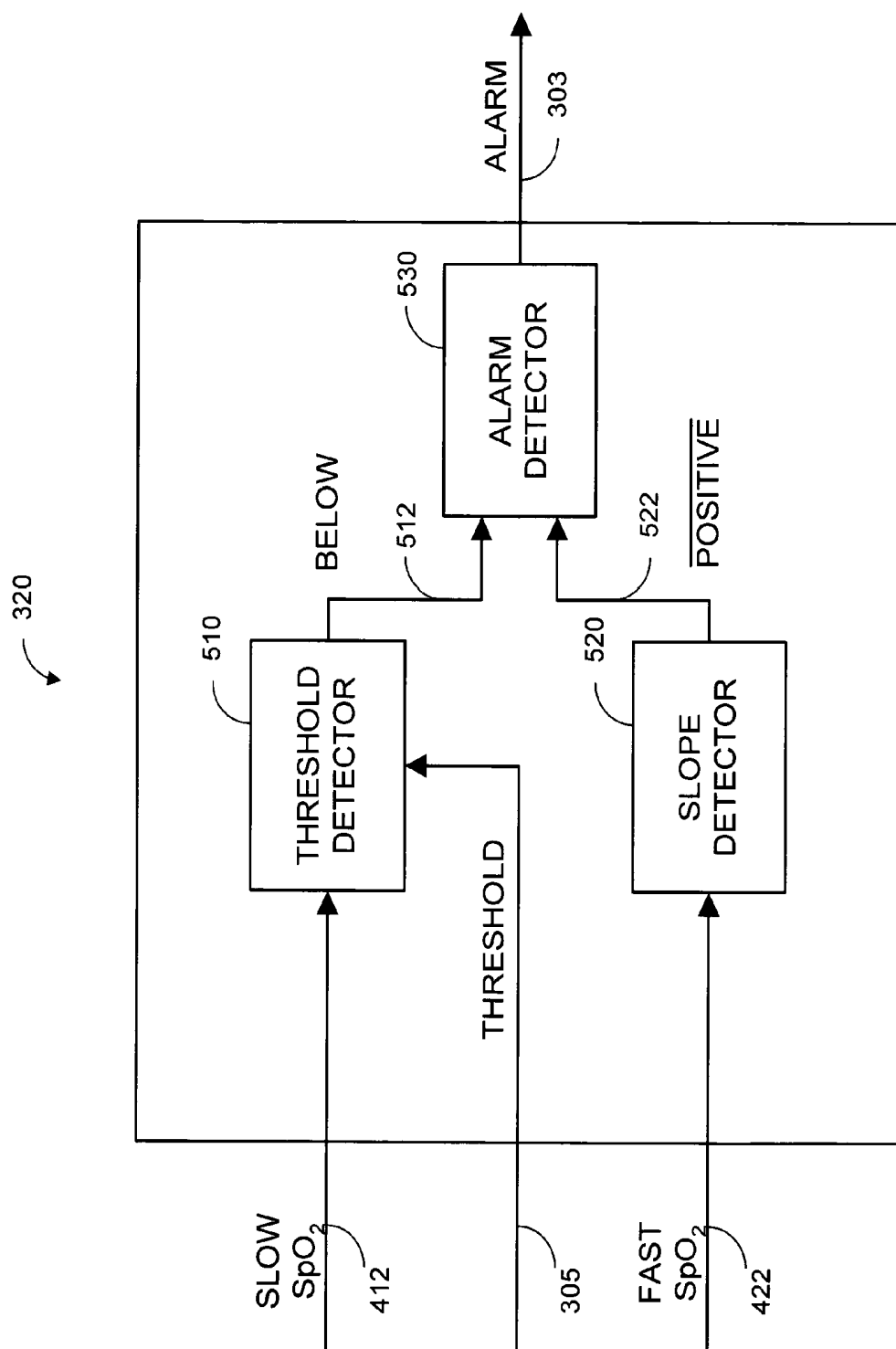


FIG. 5



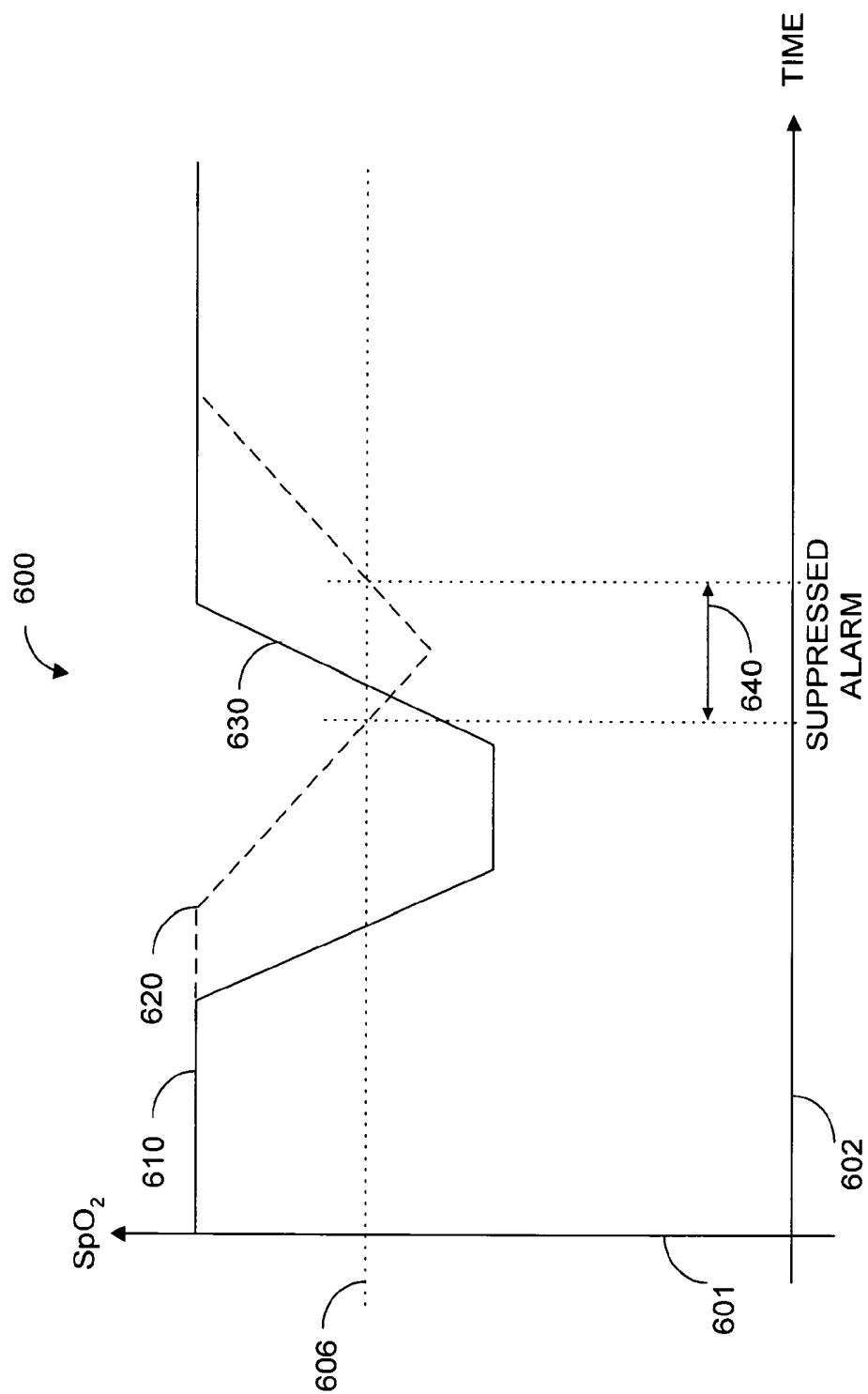


FIG. 6A

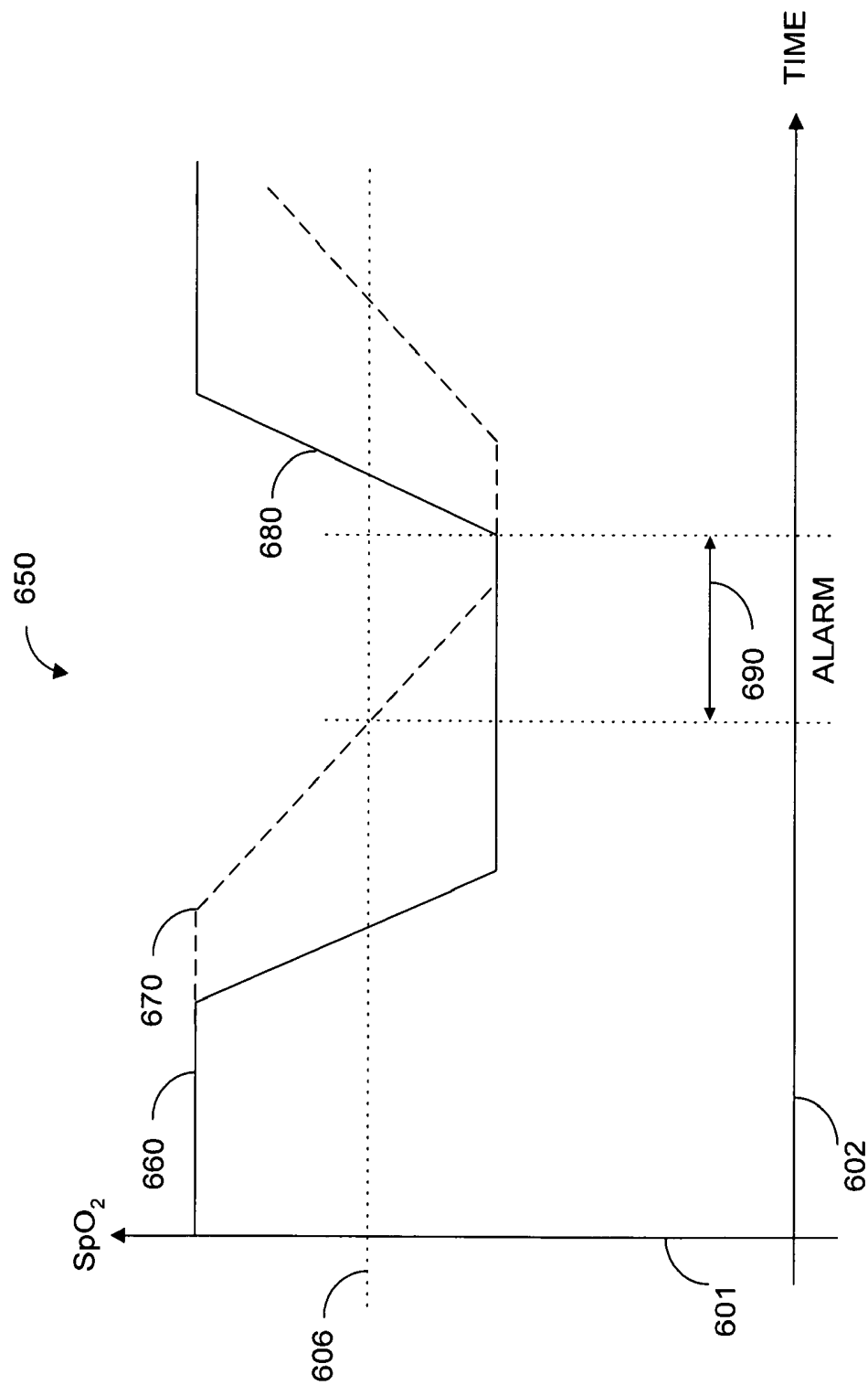


FIG. 6B

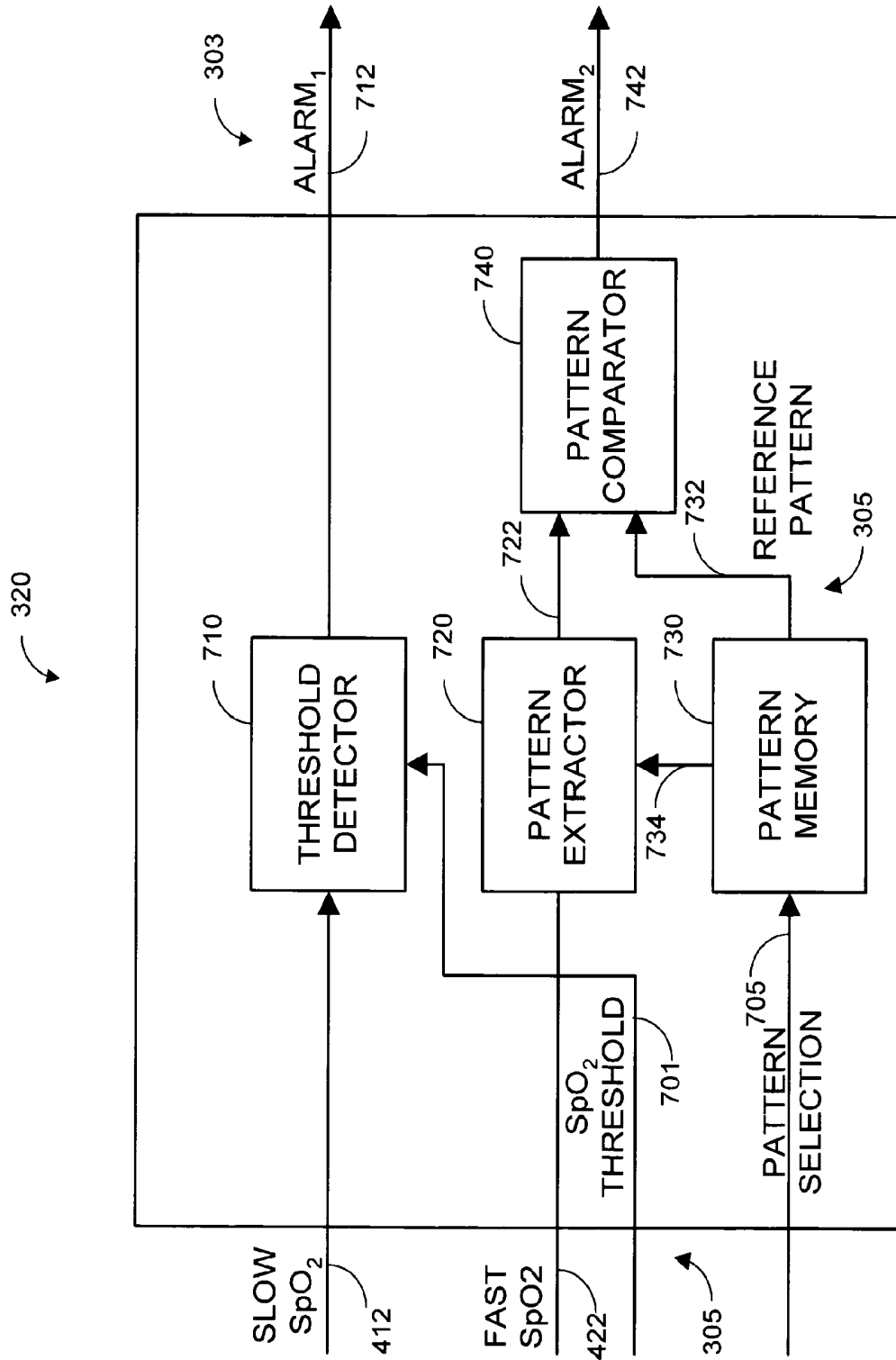


FIG. 7

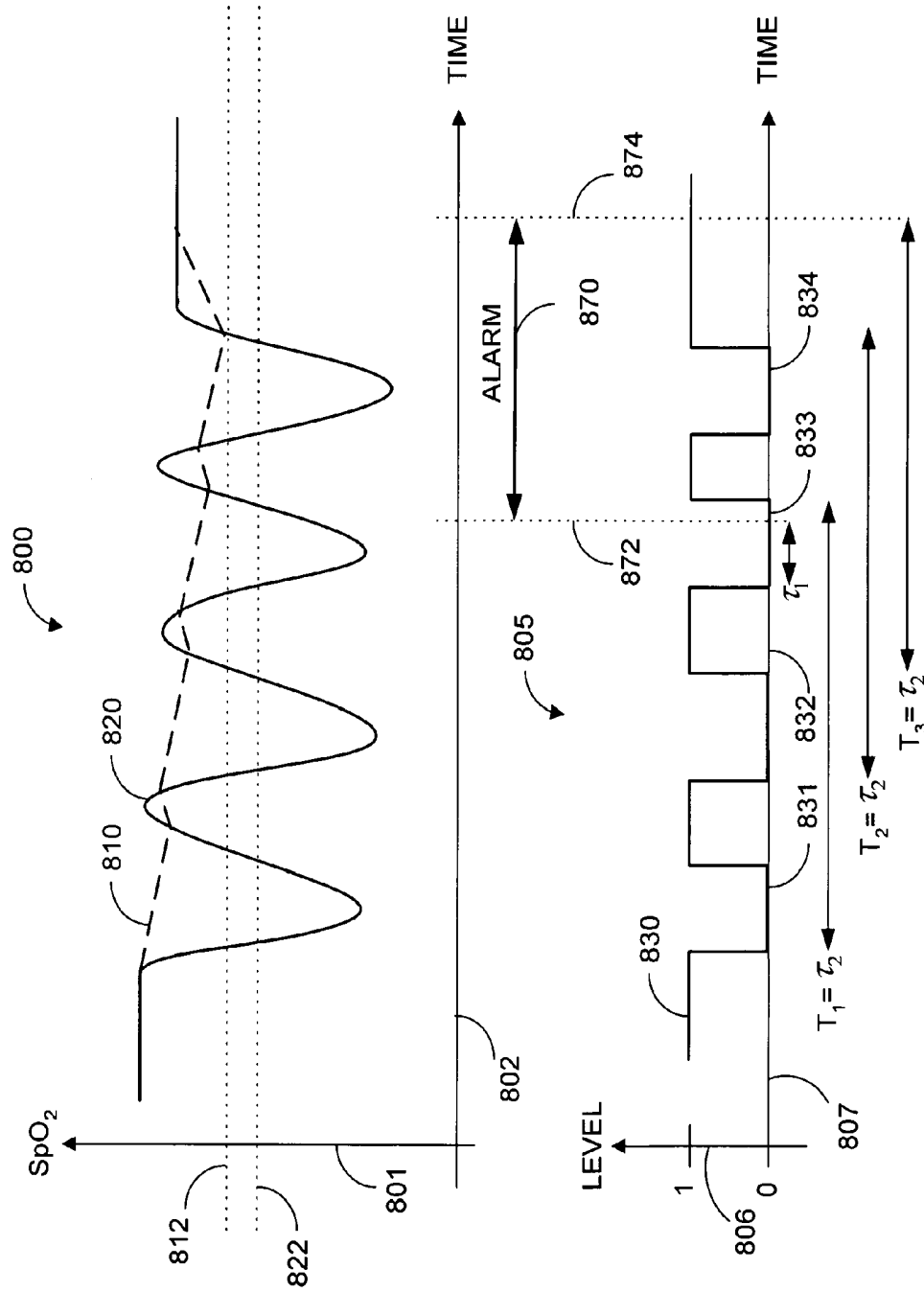


FIG. 8

## PHYSIOLOGICAL TREND MONITOR

## REFERENCE TO RELATED APPLICATIONS

The present application claims priority benefit under 35 U.S.C. §120 to, and is a continuation of U.S. patent application Ser. No. 13/018,334, filed Jan. 31, 2011 entitled "Physiological Trend Monitor," which is a continuation of U.S. patent application Ser. No. 12/070,061, filed Feb. 12, 2008, now U.S. Pat. No. 7,880,606, entitled "Physiological Trend Monitor," which is a continuation of U.S. patent application Ser. No. 11/717,591, filed Mar. 13, 2007, now U.S. Pat. No. 7,355,512, entitled "Parallel Alarm Processor," which is a continuation of U.S. patent application Ser. No. 11/405,815, filed Apr. 18, 2006, now U.S. Pat. No. 7,190,261, entitled "Arrhythmia Alarm Processor," which is a continuation of U.S. patent application Ser. No. 10/975,860, filed Oct. 28, 2004, now U.S. Pat. No. 7,030,749, entitled "Parallel Measurement Alarm Processor," which is a continuation of U.S. patent application Ser. No. 10/351,735, filed Jan. 24, 2003, now U.S. Pat. No. 6,822,564, entitled "Parallel Measurement Alarm Processor," which claims priority benefit under 35 U.S.C. §119(e) from U.S. Provisional Application No. 60/351,510, filed Jan. 24, 2002, entitled "Parallel Measurement Alarm Processor." The present application also incorporates the foregoing utility disclosures herein by reference.

## BACKGROUND OF THE INVENTION

Physiological measurement instruments employed in healthcare environments often feature visual and audible alarm mechanisms that alert a caregiver when a patient's vital signs are outside of predetermined limits. One example is a pulse oximeter, which measures the oxygen saturation level of arterial blood, an indicator of oxygen supply. A typical pulse oximeter displays a numerical readout of the patient's oxygen saturation, a numerical readout of pulse rate, and a plethysmograph, which is indicative of a patient's pulse. In addition, a pulse oximeter provides an alarm that warns of a potential desaturation event.

FIG. 1 illustrates a prior art pulse oximeter portion 100 having a signal input 101 and generating an oxygen saturation measurement output 103 and an alarm output 105. The pulse oximeter portion 100 has an oxygen saturation (SPO.sub.2) processor 110 and an associated threshold detector 120. The SPO.sub.2 processor 110 derives an oxygen saturation measurement from the signal input 101. The signal input 101 is typically an amplified, filtered, digitized and demodulated sensor signal. A sensor emits both red and infrared (IR) wavelength light, which is transmitted through a patient's tissue, detected and input to the pulse oximeter. The pulse oximeter calculates a normalized ratio (AC/DC) of the detected red and infrared intensities, and an arterial oxygen saturation value is empirically determined based on a ratio of these normalized ratios, as is well-known in the art. The oxygen saturation measurement output 103 is typically a digital signal that is then communicated to a display.

FIG. 2 illustrates the operation of a conventional threshold detector 120 (FIG. 1) utilizing a graph 200 of oxygen saturation 201 versus time 202. The graph 200 displays a particular oxygen saturation measurement 210 corresponding to the measurement output 103 (FIG. 1) and a predetermined alarm threshold 206. During an alarm time period 270 when the measured oxygen saturation 210 is below the threshold 206, an alarm output 105 (FIG. 1) is generated, which triggers a caregiver alert. Adjusting the threshold 206 to a lower value of oxygen saturation 201 reduces the probability of an alarm, i.e.

reduces the probability of a false alarm and increases the probability of a missed event. Likewise, adjusting the threshold 206 to a higher value of oxygen saturation 201 increases the probability of an alarm, i.e. increases the probability of a false alarm and decreases the probability of a missed event.

## SUMMARY OF THE INVENTION

One aspect of a physiological trend monitor comprises transmitting light into a patient tissue site, generating a sensor signal, detecting a blood parameter trend according to the sensor signal and generating an alarm according to the blood parameter trend. The transmitted light has multiple wavelengths. The sensor signal is responsive to the light after attenuation by pulsatile arterial blood flow within the tissue site. In various embodiments, the detecting comprises deriving a curve-fitting blood parameter measurement. A blood parameter slope is calculated from the blood parameter measurement. The alarm is responsive to a negative value of the blood parameter slope. A smoothed blood parameter measurement is derived. A threshold value is set for the smoothed blood parameter measurement. The alarm is responsive to the smoothed blood parameter measurement crossing the threshold value.

Another aspect of a physiological trend monitor comprises a sensor signal responsive to multiple wavelengths of light transmitted into a tissue site and detected after attenuation by pulsatile blood flow within the tissue site. A processor has an input responsive to the sensor signal and a physiological parameter output. Features are extracted from the physiological parameter output. Criteria are applied to the features. An alarm output is generated when the criteria are satisfied. In various embodiments a pattern memory stores feature values and a comparator compares the features with the stored feature values. The criteria determine a match between the features and the stored feature values so as to trigger the alarm output. At least one of the features relate to the number of threshold crossings over a specified time period. At least one of the features relate to a duration of a threshold crossing by the physiological parameter output. At least one of the features relate to a trend in the physiological parameter and a slope of that trend over a specified time period.

A further aspect of a physiological trend monitor comprises a detector responsive to multiple wavelengths of light transmitted into a tissue site after attenuation by pulsatile blood flow within the tissue site so as to generate a sensor signal. A processor means calculates a physiological measurement in response to the sensor signal. A pattern extractor means identifies features of the physiological measurement. A pattern memory means stores a reference pattern. A pattern comparator means triggers an alarm if the identified features match the reference pattern. In various embodiments, a threshold is input to the pattern extractor. The identified features comprise at least the number of times the physiological measurement crosses the threshold within a predetermined time period. The identified features comprise at least the duration of each time the physiological measurement crosses the threshold. The physiological measurement comprises a predictive oxygen saturation measurement. A second processor means calculates an integrator oxygen saturation measurement.

## BRIEF DESCRIPTION OF THE DRAWINGS

FIG. 1 is a block diagram of a prior art pulse oximeter portion;

FIG. 2 is a graph of oxygen saturation versus time illustrating a conventional threshold detector alarm;

FIG. 3 is a block diagram of an alarm processor utilizing parallel measurements of a physiological parameter;

FIG. 4 is a block diagram of a pulse oximeter processor utilizing dual oxygen saturation measurements;

FIG. 5 is a block diagram of a predictive alarm indicator utilizing a threshold detector with a slow oxygen saturation measurement input and a slope detector with a fast oxygen saturation measurement input;

FIGS. 6A-B are graphs of oxygen saturation versus time illustrating operation of the alarm indicator according to FIG. 5;

FIG. 7 is a block diagram of a pattern recognition alarm indicator utilizing a threshold detector with a slow oxygen saturation measurement input and a pattern extractor with a fast oxygen saturation measurement input; and

FIG. 8 is a graph of oxygen saturation versus time illustrating the pattern recognition alarm indicator according to FIG. 7.

#### DETAILED DESCRIPTION OF THE PREFERRED EMBODIMENTS

FIG. 3 illustrates a parallel measurement alarm processor 300. The alarm processor 300 has a sensor signal input 301 responsive to a physiological parameter and provides one or more alarm outputs 303 to indicate that the physiological parameter may have exceeded particular limits. The alarm processor 300 also has multiple parameter processors 310, which do not necessarily have the same or similar internal configurations. The multiple parameter processors 310 input the sensor signal 301 and provide parallel measurements 312 of the physiological parameter, each measurement having differing characteristics, such as response time or bandwidth to name a few. The alarm processor 300 further has an alarm indicator 320 that inputs the parallel parameter measurements 312 and generates the alarm outputs 303 based upon alarm conditions 305. The alarm outputs 303 change state to indicate that the parameter may have exceed one or more limits and to trigger an alarm accordingly. The alarm conditions 305 define particular limits with respect to one or more of the measurements 312. The alarm conditions 305 may be pre-defined, such as by user input, or determined by a separate process, such as a measurement of sensor signal quality or data confidence as described in U.S. patent application Ser. No. 09/858,114 entitled "Pulse Oximetry Data Confidence Indicator," assigned to Masimo Corporation, Irvine, Calif. and incorporated by reference herein. The alarm processor 300 may also have a display driver 330 that processes one or more of the parameter measurements 312 and provides one or more display, outputs 307.

FIG. 4 illustrates a pulse oximeter embodiment 400 of the alarm processor 300 (FIG. 3) described above. A pulse oximeter sensor (not shown) provides a signal input 301 that is responsive to arterial oxygen saturation, as described with respect to FIG. 1, above. The alarm processor 400 has dual oxygen saturation processors 310. An integrator oxygen saturation (SpO.sub.2) processor 410 outputs a slow SpO.sub.2 measurement 412, i.e. a measurement having a slow response time to changes in the SpO.sub.2 parameter. A predictor SpO.sub.2 processor 420 outputs a fast SpO.sub.2 measurement 422, i.e. a measurement having a fast response time that tracks changes in the SpO.sub.2 parameter. The slow SpO.sub.2 measurement 412 is input to a display driver 330, which provides an oxygen saturation display output 307. For example, the display output 307 may be input to a digital

display that provides a numerical readout of oxygen saturation to a caregiver. Both the slow SpO.sub.2 measurement 412 and the fast SpO.sub.2 measurement 422 are input to an alarm indicator 320 that generates at least one alarm output 303 based upon alarm conditions 305, as described in further detail with respect to FIGS. 5-8, below.

The integrator SpO.sub.2 processor 410, advantageously, provides a smoothed measurement of oxygen saturation suitable for threshold detection. The predictor SpO.sub.2 processor 420, advantageously, provides a curve-fitting or a predictive measurement of oxygen saturation that detects trends in oxygen saturation, as described in further detail with respect to FIG. 5 and FIGS. 6A-B, below. Further, the predictor SpO.sub.2 processor 420 advantageously tracks oxygen saturation details that may signal a critical physiological event, as described in further detail with respect to FIGS. 7-8, below. The integrator SpO.sub.2 processor 410 and predictor SpO.sub.2 processor 420 may be a pulse oximeter as described in U.S. patent application Ser. No. 09/586,845 entitled "Variable Mode Averager," assigned to Masimo Corporation, Irvine, Calif. and incorporated by reference herein.

FIG. 5 illustrates a trend embodiment of an alarm indicator 320, which has a threshold detector 510, a slope detector 520 and alarm detector 530. The threshold detector 510 has a slow SpO.sub.2 measurement 412 and a threshold alarm condition 305 as inputs and a logic output BELOW 512. The slope detector 520 has a fast SpO.sub.2 measurement 422 input and a logic output POSITIVE/522. The alarm detector 530 has BELOW 512 and POSITIVE/522 logic inputs and generates an alarm output 303. The threshold detector 510 is a comparator that asserts BELOW 512 while the slow SpO.sub.2 measurement 412 is less in value than the value of the threshold 305. The slope detector 520 is a differentiator and comparator that asserts POSITIVE/522 while the slope of the fast SpO.sub.2 measurement 422 is non-positive, i.e. while the derivative of the fast SpO.sub.2 measurement 422 is zero or less than zero. The alarm detector 530 performs a logical AND function, asserts the alarm output 303 and indicates an alarm when BELOW 512 and POSITIVE/522 are both asserted. In this manner, an alarm output 303 only changes state when the slow SpO.sub.2 measurement 412 is below a threshold 305 and the fast SpO.sub.2 measurement 422 has not begun to increase in value. Advantageously, the trend recognition alarm indicator 320 reduces false alarms by suppressing a threshold-based alarm on the slow SpO.sub.2 measurement 412 when the fast SpO.sub.2 measurement 422 determines that a patient's oxygen saturation is in recovery, as described in further detail with respect to FIGS. 6A-B, below.

FIGS. 6A-B illustrate operation of the trend recognition alarm indicator 320 (FIG. 5). In FIG. 6A, a graph 600 has an SpO.sub.2 axis 601 and a time axis 602. Shown along the SpO.sub.2 axis 601 is a constant SpO.sub.2 value 606 corresponding to a threshold 305 (FIG. 5). The graph 600 shows a first plot of SpO.sub.2 versus time 610 corresponding to a fast SpO.sub.2 measurement 422 (FIG. 5). The graph 600 also shows a second plot of SpO.sub.2 versus time 620 corresponding to a slow SpO.sub.2 measurement 412 (FIG. 5). A suppressed alarm interval 640 along the time axis 602 corresponds to an alarm that would be indicated by the threshold detector 510 (FIG. 5) but is suppressed as occurring during a positive slope portion 630 of a fast SpO.sub.2 measurement 610. The alarm detector 530 (FIG. 5) would not assert an alarm output 303 (FIG. 5) during this interval.

In FIG. 6B, a graph 650 shows a first plot of SpO.sub.2 versus time 660 corresponding to a fast SpO.sub.2 measurement 422 (FIG. 5). The graph 650 also shows a second plot of SpO.sub.2 versus time 670 corresponding to a slow SpO-

.sub.2 measurement **412** (FIG. 5). An alarm interval **690** along the time axis **602** corresponds to an alarm period triggered by the alarm output **303** (FIG. 5). This alarm interval **640** occurs while a slow SpO.sub.2 measurement **670** is below the threshold **606** and before a positive slope portion **680** of a fast SpO.sub.2 measurement **660**.

FIG. 7 illustrates a pattern recognition embodiment of an alarm indicator **320**, having a threshold detector **710**, a pattern extractor **720**, a pattern memory **730** and a pattern comparator **740**. Further, the alarm indicator **320** has slow SpO.sub.2 **412** and fast SpO.sub.2 **422** measurement inputs in addition to a threshold **701** input and a pattern selection in **705** as alarm condition inputs **305**. The threshold detector **710** has a slow SPO.sub.2 measurement **412** and a SpO.sub.2 threshold **701** as inputs and a first alarm output **712**. The threshold detector **710** changes the state of the first alarm output **712** when the value of the slow SpO.sub.2 measurement **412** crosses the SpO.sub.2 threshold **701**. For example, the first alarm output **712** changes state to trigger an alarm when the slow SpO.sub.2 measurement **412** becomes less than the SpO.sub.2 threshold **701**.

As shown in FIG. 7, the pattern extractor **720** has a fast SpO.sub.2 measurement **422** and a pattern threshold **734** as inputs and an extracted pattern output **722**. The pattern extractor **720** identifies features of the fast SpO.sub.2 measurement **422** that may be used for pattern matching. Features may be, for example, the number of times the fast SpO.sub.2 measurement **422** crosses the pattern threshold **734** within a certain time period, or the duration of each time period that the fast SpO.sub.2 measurement **422** is less than the pattern threshold **734**, to name a few. The pattern memory **730** has a pattern selection input **705** and a reference pattern output **732**. The pattern memory **730** stores values for particular features that are identified by the pattern extractor **720**. The reference pattern output **732** transfers these stored values to the pattern comparator **740**. The pattern memory **730** may be nonvolatile and one or more patterns may be stored at the time of manufacture or downloaded subsequently via a data input (not shown). One of multiple patterns may be determined via the pattern selection input **705**, by a user or by a separate process, for example. The pattern threshold **734** may be generated in response to the pattern selection input **705** or in conjunction with a selected reference pattern **732**.

Also shown in FIG. 7, the pattern comparator **740** has the extracted pattern **722** and the reference pattern **732** as inputs and generates a second alarm output **742**. That is, the pattern comparator **740** matches extracted measurement features provided by the pattern extractor **720** with selected features retrieved from pattern memory **730**, changing the state of the second alarm output **742** accordingly. For example, the second alarm output **742** changes state to trigger an alarm when features of the fast SpO.sub.2 measurement **422** match the reference pattern output **732**. Advantageously, the pattern recognition alarm indicator **320** reduces missed events by supplementing the threshold-based first alarm output **712** responsive to the slow SpO.sub.2 measurement **412** with a pattern-based second alarm output **742** responsive to detail in the fast SpO.sub.2 measurement **422**. In this manner, if a patient's oxygen saturation is, for example, irregular or intermittent, the second alarm output **742** may trigger a caregiver alert when the first alarm output **712** does not, as described in further detail with respect to FIG. 8, below.

FIG. 8 illustrates operation of a pattern recognition alarm indicator **320** (FIG. 7), as described above. A graph **800** has a SpO.sub.2 axis **801** and a time axis **802**. The graph **800** shows a SpO.sub.2 plot versus time **810** corresponding to the slow SPO.sub.2 measurement **412** (FIG. 7). Shown along the time

axis **802** is a constant SPO.sub.2 value **812** corresponding to the SPO.sub.2 threshold **701** (FIG. 7). Due to the short duration of irregular and intermittent drops in SpO.sub.2, the slow SpO.sub.2 measurement **810** does not fall below the SpO.sub.2 threshold **812**. Thus, the first alarm output **712** (FIG. 7) does not trigger an alarm in this example.

Also shown in FIG. 8, the graph **800** shows a SpO.sub.2 plot versus time **820** corresponding to the fast SpO.sub.2 measurement **422** (FIG. 7). Shown along the time axis **802** is a constant SPO.sub.2 value **822** corresponding to the pattern threshold **734** (FIG. 7). A corresponding graph **805** has a logic level axis **806** and a time axis **807**. The graph **805** shows a logic level plot versus time **830** corresponding to the extracted pattern output **722** (FIG. 7). The logic level plot **830** has a "1" level when the fast SpO.sub.2 plot **820** is above the pattern threshold **822** and a "0" level when the fast SpO.sub.2 plot **820** is below the pattern threshold **822**. In this manner, the logic level plot **830** indicates the number and duration of times the fast SpO.sub.2 plot **820** falls below a threshold value **822**.

Further shown in FIG. 8, an alarm interval **870** along the time axis **802** corresponds to an alarm period indicated by the pattern comparator **740** (FIG. 7). This alarm interval **870** occurs after a reference pattern **732** (FIG. 7) is detected as matching an extracted pattern **722** (FIG. 7) and ends, correspondingly, when there is no longer a match. For example, assume that the reference pattern output **732** (FIG. 7) has the alarm criteria that at least three below threshold periods of minimum duration T.sub.1 must occur during a maximum period T.sub.2, where the value of T.sub.1 and T.sub.2 are illustrated along the time axis **807**. The below threshold time periods **831-834** are each greater in duration than T.sub.2 and a first set of three, below-threshold time periods **831-833** occurs within a time period T.sub.1=T.sub.2, as illustrated. Thus, the alarm interval beginning **872** is triggered by the second alarm output **742** (FIG. 7). A second set of three, below-threshold time periods **832-834** also occurs within a time period T.sub.2=T.sub.2, as illustrated. Thus, the alarm interval **870** continues. There is no third set of three, below-threshold time periods. Thus, after the end of the time interval T.sub.3=T.sub.2, the alarm interval end **874** is triggered. This example illustrates how the pattern recognition alarm indicator **320** (FIG. 7) can trigger an alarm on an event, such as a period of irregular heartbeats, that might be missed by a threshold-based alarm responsive to the slow SpO.sub.2 measurement **412**.

Although some alarm processor embodiments were described above in terms of pulse oximetry and oxygen saturation measurements, one of ordinary skill in the art will recognize that an alarm processor as disclosed herein is also applicable to the measurement and monitoring of other blood constituents, for example blood glucose and total hemoglobin concentration to name a few, and other physiological parameters such as blood pressure, pulse rate, respiration rate, and EKG to name a few.

In an embodiment, multiple pattern processors, each including a pattern extractor, pattern memory and pattern comparator, such as described with respect to FIG. 7, above, have as inputs one or more of fast SpO.sub.2 measurements, a pulse oximeter plethysmograph and pulse rate measurements. An arrhythmia alarm is generated based upon irregular heartbeat patterns being matched or otherwise detected in one or more combinations of SpO.sub.2 measurements, a pulse oximeter plethysmograph and pulse rate measurements.

A physiological trend monitor has been disclosed in detail in connection with various embodiments. These embodiments are disclosed by way of examples only and are not to

limit the scope of the claims that follow. One of ordinary skill in the art will appreciate many variations and modifications.

What is claimed is:

1. A patient monitor configured to receive sensor signals from an optical sensor responsive to attenuation of light by body tissue at a measurement site, the monitor comprising:
  - a processor determining measurement values of a physiological parameter, said measurement values responsive to said sensor signals;
  - an alarm indicator receiving smoothed values of said measurement values of said physiological parameter and receiving predictive values of said measurement values of said physiological parameter;
  - an alarm; and
  - a memory storing first and second criteria, each indicative of alarm conditions, said first criteria being relevant to said smoothed values and said second criteria being relevant to said predictive values,
 said alarm indicator comparing features to said first criteria, and when said features match said first criteria, triggering said alarm, and
  - said alarm indicator comparing features to said second criteria, and when said features match said second criteria, triggering said alarm.
2. The monitor according to claim 1 wherein said processor includes a plurality of parallel processing modules, each responsive to said sensor signals, at least one module having different characteristics from another module, at least one of said modules outputting said smoothed values and another of said modules outputting said predictive values.
3. The monitor according to claim 1 wherein said physiological parameter comprises oxygen saturation.
4. The monitor according to claim 1 wherein said physiological parameter comprises glucose.
5. The monitor according to claim 1 wherein said physiological parameter comprises total hemoglobin.
6. The monitor according to claim 1 wherein said physiological parameter comprises blood pressure.
7. The monitor according to claim 1 wherein said physiological parameter comprises pulse rate.
8. The monitor according to claim 1 wherein said physiological parameter comprises respiration rate.
9. The monitor according to claim 1 wherein said physiological parameter comprises EKG data.
10. A method of triggering an alarm to alert a caregiver of a need for attention to a patient wearing a patient monitor configured to receive sensor signals from an optical sensor responsive to attenuation of light by body tissue of said patient, the method comprising:
  - determining measurement values of a physiological parameter with a processor, said measurement values responsive to said sensor signals;
  - receiving smoothed values of said measurement values of said physiological parameter;
  - receiving predictive values of said measurement values of said physiological parameter;
  - storing first and second criteria, each indicative of alarm conditions, said first criteria being relevant to said smoothed values and said second criteria being relevant to said predictive values;
  - comparing features to said first criteria;
  - when said features match said first criteria, triggering said alarm;
  - comparing features to said second criteria; and

when said features match said second criteria, triggering said alarm.

11. The method according to claim 10 wherein determining includes parallel processing said sensor signals where at least one processing method includes different characteristics from another, at least one of said processing methods determines said smoothed values and another determines said predictive values.

12. The method according to claim 10 wherein said determining measurement values of said physiological parameter comprises determining measurement values of oxygen saturation.

13. The method according to claim 10 wherein said determining measurement values of said physiological parameter comprises determining measurement values of glucose.

14. The method according to claim 10 wherein said determining measurement values of said physiological parameter comprises determining measurement values of total hemoglobin.

15. The method according to claim 10 wherein said determining measurement values of said physiological parameter comprises determining measurement values of blood pressure.

16. The method according to claim 10 wherein said determining measurement values of said physiological parameter comprises determining measurement values of pulse rate.

17. The method according to claim 10 wherein said determining measurement values of said physiological parameter comprises determining measurement values of respiration rate.

18. The method according to claim 10 wherein said determining measurement values of said physiological parameter comprises determining measurement values of EKG data.

19. A parallel alarm for a patient monitor, said patient monitor configured to receive sensor signals from a sensor responsive to attenuation of light by body tissue, the parallel alarm comprising:

- a memory;
- an alarm activating upon receiving an alarm trigger;
- a threshold detector receiving relatively slow changing physiological parameter data response to said sensor signals, electronically comparing said relatively slow changing physiological parameter data to threshold data stored in said memory, and outputting said alarm trigger when said relatively slow changing physiological parameter data compares with said threshold data in a predetermined manner; and
- a pattern comparator receiving relatively fast changing physiological parameter data response to said sensor signals, electronically comparing said relatively fast changing physiological parameter data to pattern data stored in said memory, and outputting said alarm trigger when said relatively fast changing physiological parameter data compares with said pattern data in a predetermined manner.

20. The parallel alarm according to claim 19, comprising a plurality of parallel processing modules, each responsive to said sensor signals, at least one module having different characteristics from another module, at least one of said modules outputting relatively slow changing physiological parameter data and another of said modules outputting relatively fast changing physiological parameter data.



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#### 摘要(译)

生理趋势监测器具有响应于传输到组织部位的多个波长的光的传感器信号。在通过组织部位内的脉动血流衰减后检测透射光。处理器具有响应于传感器信号和生理参数输出的输入。从生理参数输出中提取特征。标准适用于特征。满足条件时生成警报输出。

