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(54) **APPARATUS, COMPUTER SYSTEM AND COMPUTER PROGRAM FOR DETERMINING INTRATHORACIC BLOOD VOLUME AND OTHER CARDIO-VASCULAR PARAMETERS**

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(57) **ABSTRACT**

Apparatus, computer system, computer program and storage medium for determining intrathoracic blood volume (ITBV) and other cardio-vascular parameters of a patient by thermodilution measurements. The apparatus comprises

a) temperature influencing means (107) for provoking an initial local temperature change in the proximity of a first place (101) of a patient's vascular system (103), thus introducing a travelling temperature deviation to patient's blood stream,

b) a temperature sensor device (117) for measuring the local temperature of patient's blood at a second place (102) of patient's vascular system (103) downstream of said first place (101)

c) a computer system (104) coupled to said temperature sensor device (117) and adapted to record said patient's local blood temperature measured at said second place (102) as a function of time to determine a thermodilution curve,

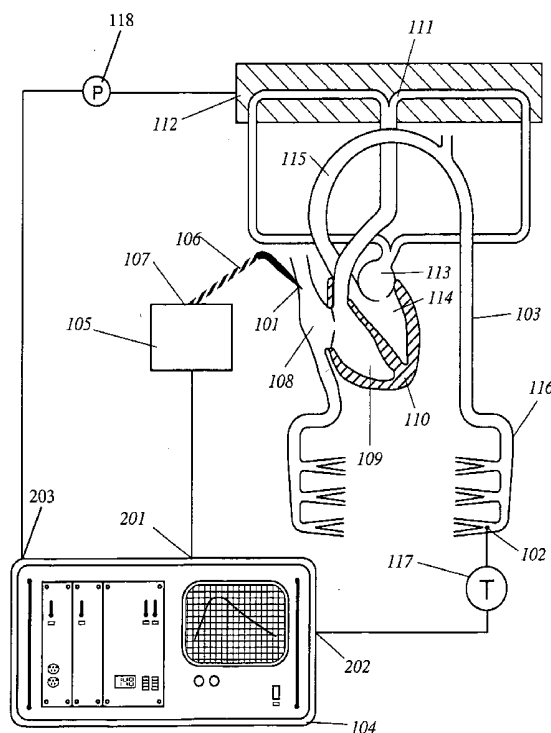
d) said computer system (104) being further adapted to determine patient's global enddiastolic blood volume (GEDV) and patient's intrathoracic thermovolume (ITTV) from said thermodilution curve,

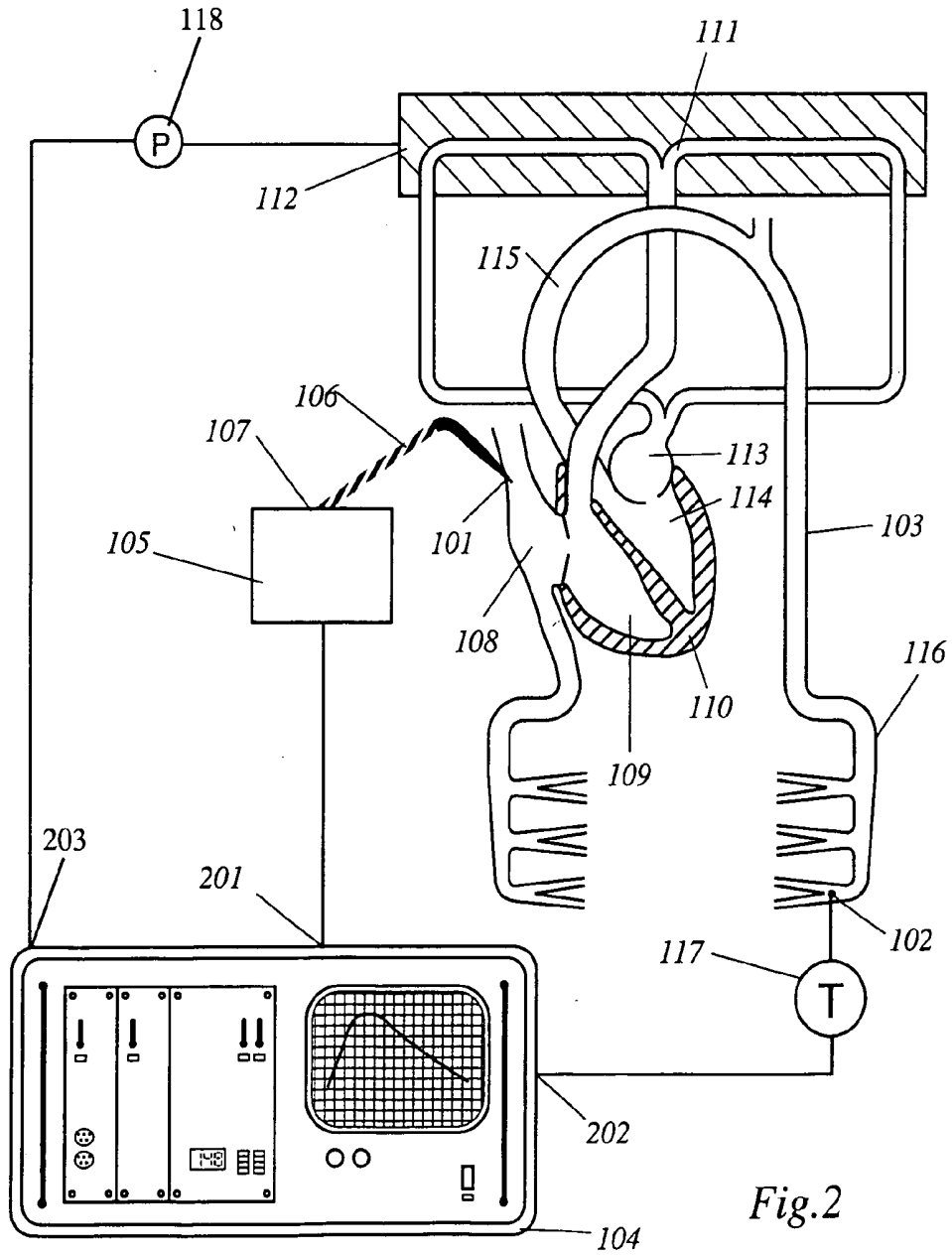
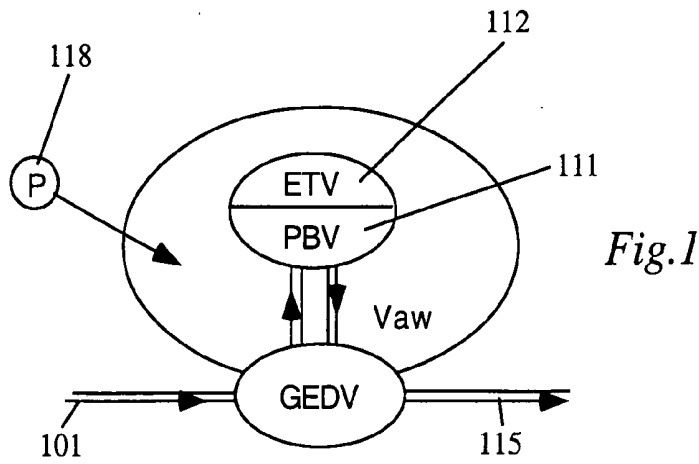
e) said computer system (104) being further adapted to determine patient's intrathoracic blood volume (ITBV) according to the following formula:

$$ITBV=f(GEDV, ITTV, P),$$

ITBV being the intrathoracic blood volume, GEDV being the global enddiastolic blood volume, ITTV being the intrathoracic thermovolume, P being an airway pressure inside patient's lungs.

By determining ITBV not only from GEDV but also as a function of ITTV and P enhanced accuracy can be obtained, especially if the patient suffers from pulmonary edema and/or is mechanically ventilated.





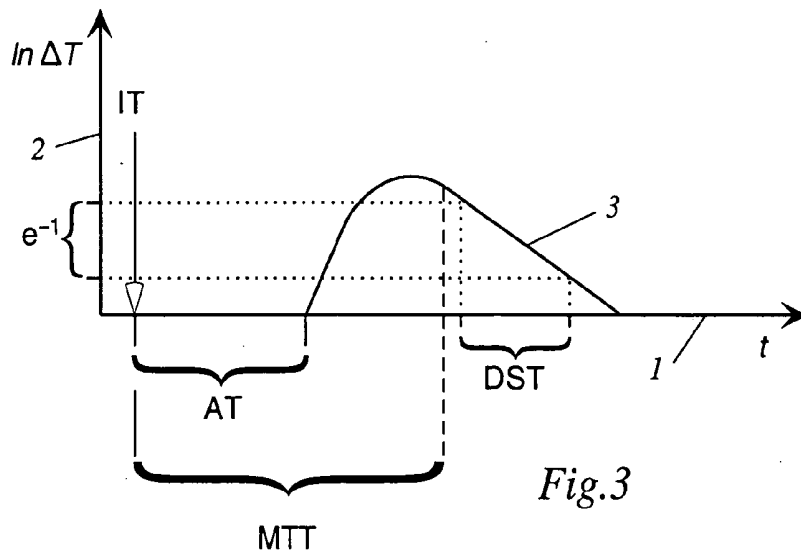


Fig.3

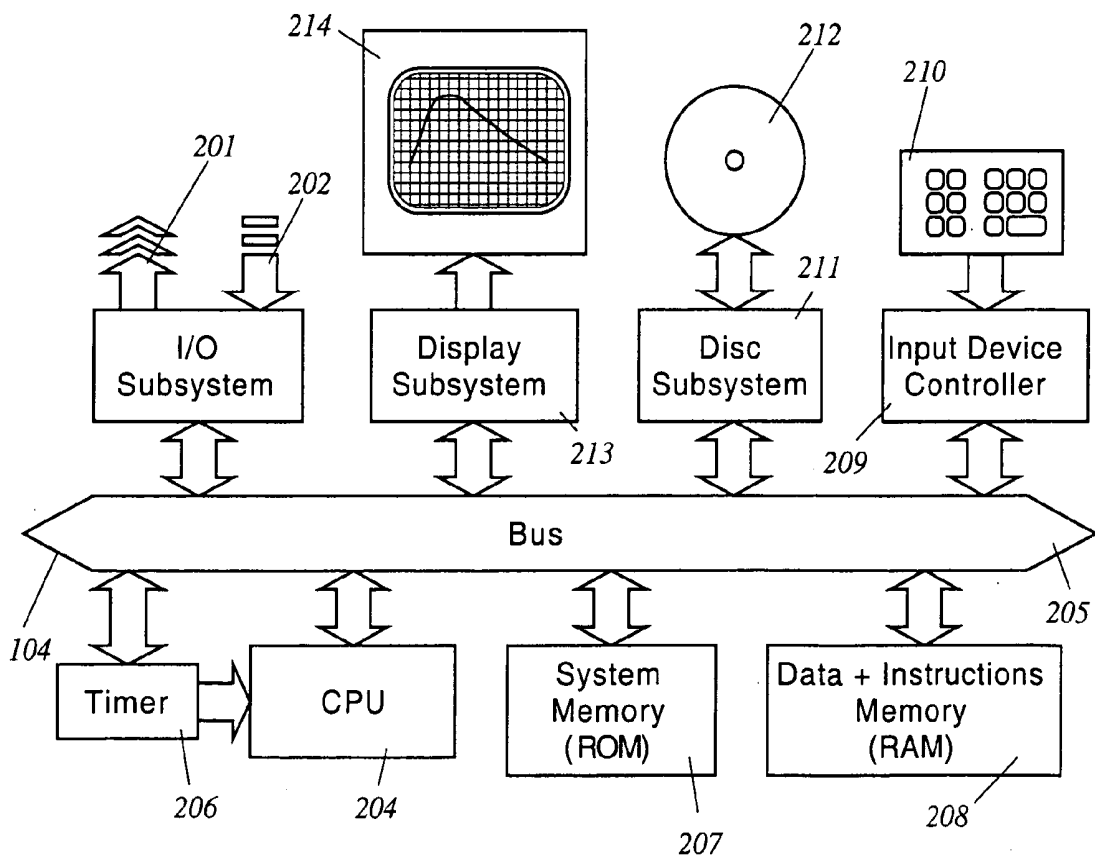


Fig.4

**APPARATUS, COMPUTER SYSTEM AND
COMPUTER PROGRAM FOR DETERMINING
INTRATHORACIC BLOOD VOLUME AND OTHER
CARDIO-VASCULAR PARAMETERS**

FIELD OF THE INVENTION

[0001] The present invention relates to an apparatus, a computer system and a computer program for determining intrathoracic blood volume and other cardiovascular parameters of a patient by thermodilution measurements.

BACKGROUND OF THE INVENTION

[0002] The current state of the art in implementing transpulmonary thermodilution measurement are apparatus for injecting a bolus of thermal indicator into a patient's vena cava superior, and measuring the temperature response at a place of the patient's systemic circulation, e.g. patient's femoral artery to determine the thermodilution curve, i.e. the temperature response as a function of time. From the thermodilution curve, a schematic example of which is illustrated in **FIG. 3**, wherein the abscissa (time axis) 1 is linear and the ordinate (temperature difference axis) 2 is logarithmic, various cardio-vascular parameters can be derived by using computer systems running computer programs, which implement parameter calculations as disclosed in WO 93/21823, the contents of which are included herein by citation, and as set forth briefly below.

[0003] The Cardiac Output CO can be determined by algorithms based on the Stewart-Hamilton-equation:

$$CO = \frac{V_L(T_B - T_L)K_1K_2}{\int_{\Delta T_B(t)} dt}$$

[0004] where T_B is the initial blood temperature, T_L is the temperature of the liquid bolus, which is used as thermal indicator, V_L is the thermal indicator volume, K_1 and K_2 are constants to consider the specific measurement setup, and $\Delta T_B(t)$ is the blood temperature as a function of time with respect to the baseline blood temperature T_B . Thermal indicator can either be colder or warmer with respect to blood temperature. To obtain cardiac output, the area under the thermodilution curve has to be determined by mathematical integration.

[0005] Other parameters that can be derived from the thermodilution curve **3** as schematically illustrated in **FIG. 1** include the Exponential Decay or Downslope Time DST, i.e. the time the blood temperature difference $\Delta T_B(t)$ takes to drop by the factor e^{-1} , the Appearance Time AT, i.e. the time span between bolus injection IT and first appearance of a noticeable temperature difference $\Delta T_B(t)$ and the Mean Transit Time MTT.

[0006] The Intrathoracic Thermovolume ITTV and the Intrathoracic blood volume ITBV can be determined as follows:

$$ITTV = CO \cdot MIT$$

$$ITBV = a' \cdot GEDV + b'$$

[0007] wherein a' and b' are species-specific constants and GEDV is the Global End-Diastolic Volume, which can be determined as follows:

$$GEDV = CO \cdot (MIT - DST)$$

[0008] An extravascular thermovolume estimate can be determined as the difference between Intrathoracic Thermovolume ITTV and the Intrathoracic blood volume ITBV

$$ETV = ITTV - ITBV$$

[0009] Extravascular thermovolume correlates, if there is no significant perfusion defect in the lungs (e.g. massive pulmonary embolism or large single embolism), closely to the degree of Extravascular Lung Water.

[0010] Transpulmonary thermodilution has been shown to be a reliable technique for assessing cardiac output, cardiac preload and extravascular lung water (EVLW), i.e. to quantify pulmonary edema. The estimation of EVLW by the injection of a single thermal indicator is based on the above mentioned relationship $ITBV = a' \cdot GEDV + b'$. This method has been shown to compare favorably with the double-indicator (thermo-dye) dilution technique and with the ex-vivo gravimetric methods.

[0011] However, for mechanically ventilated patients and patients suffering from severe pulmonary edema the results were not entirely satisfactory.

[0012] It is therefore an object of the present invention to provide a new apparatus, a new computer system and a new computer program allowing the determination of the intrathoracic blood volume by single indicator transpulmonary thermodilution with enhanced accuracy especially for patients suffering from severe pulmonary edema and/or for mechanically ventilated patients.

SUMMARY OF THE INVENTION

[0013] The inventors found that several factors (especially pulmonary edema and airway pressure) affect the cardiac blood/pulmonary blood volume relationship, and hence the estimation of EVLW by transpulmonary thermodilution. Indeed, edematous lung areas may compress pulmonary vessels and enhance pulmonary vasoconstriction, both factors that may reduce true pulmonary blood volume and hence lead to overestimation of ITBV and under-estimation of extravascular lung water EVLW (when ITBV is estimated as $1.25 \times GEDV$). Similarly, any increase in airway pressure (related either to an increase in tidal volume or the application of a positive end-expiratory pressure) may induce a decrease in pulmonary blood volume which may also change the cardiac/pulmonary blood volume ratio.

[0014] In order to accomplish the above mentioned object, the present invention provides an apparatus for determining intrathoracic blood volume (ITBV) and other cardio-vascular parameters of a patient by thermodilution measurements comprising: temperature influencing means for provoking an initial local temperature change in the proximity of a first place of a patient's vascular system, thus introducing a travelling temperature deviation to patient's blood stream, a temperature sensor device for measuring the local temperature of patient's blood at a second place of patient's vascular system downstream of said first place, a computer system connected to said temperature sensor device and adapted to record said patient's local blood temperature measured at said second place as a function of time to determine a thermodilution curve, said computer system being further adapted to determine patient's global enddiastolic blood volume (GEDV) and patient's intrathoracic thermovolume

(ITTV) from said thermodilution curve said computer system being further adapted to determine patient's intrathoracic blood volume (ITBV) according to the following formula:

$$ITBV=f(GEDV, ITTV, P)$$

[0015] ITBV being the intrathoracic blood volume, GEDV being the global enddiastolic blood volume, ITTV being the intrathoracic thermovolume, P being an airway pressure inside patient's lungs.

[0016] In order to accomplish the above mentioned object, the invention also provides a computer system comprising first coupling means to couple said computer system to temperature influencing means and second coupling means to couple said computer system to a temperature sensor device and optionally third coupling means to couple said computer system to an airway pressure sensor device, and accessing means to access executable instructions to cause said computer system to control temperature influencing means for provoking an initial local temperature change in the proximity of a first place of a patient's vascular system, thus introducing a temperature deviation to patient's blood stream, to record said patient's local blood temperature measured by a temperature sensor device for measuring the local temperature of patient's blood at a second place of patient's vascular system downstream of said first place as a function of time to determine a thermodilution curve, to determine patient's global enddiastolic blood volume (GEDV) and patient's intra-thoracic thermovolume (ITTV) from said thermodilution curve, to determine patient's intrathoracic blood volume (ITBV) according to the following formula:

$$ITBV=f(GEDV, ITTV, P),$$

[0017] ITBV being the intrathoracic blood volume, GEDV being the global enddiastolic blood volume, ITTV being the intrathoracic thermovolume, P being an airway pressure inside patient's lungs.

[0018] In order to accomplish the above mentioned object, the invention also provides a computer program for determining intrathoracic blood volume (ITBV) and other cardio-vascular parameters of a patient by thermodilution measurements comprising instructions executable by a computer system to cause said computer system to control temperature influencing means for provoking an initial local temperature change in the proximity of a first place of a patient's vascular system, thus introducing a temperature deviation to patient's blood stream, to record said patient's local blood temperature measured by a temperature sensor device for measuring the local temperature of patient's blood at a second place of patient's vascular system downstream of said first place as a function of time to determine a thermodilution curve, to determine patient's global enddiastolic blood volume (GEDV) and patient's intrathoracic thermovolume (ITTV) from said thermodilution curve, to determine patient's intrathoracic blood volume (ITBV) according to the following formula:

$$ITBV=f(GEDV, ITTV, P),$$

[0019] ITBV being the intrathoracic blood volume, GEDV being the global enddiastolic blood volume, ITTV being the intrathoracic thermovolume, P being an airway pressure inside patient's lungs.

[0020] By determining intrathoracic blood volume not only as a function of the global enddiastolic blood volume (GEDV) but also as a function of the intrathoracic thermovolume, experience has shown that a better estimation of intrathoracic blood volume and hence also a better estimation of extravasal lung water can be made.

[0021] According to a preferred embodiment of the invention said function $f(GEDV, ITTV, P)$ is selected to be

$$f(GEDV, ITTV, P)=a \cdot GEDV+b+c \cdot ITTV+d \cdot P$$

[0022] a being a species dependent parameter, with $1 < a < 2$, b being a species dependent parameter, including zero, c being a species dependent parameter, with c and d being species dependent parameters, including zero, with the limitation that c and d may not be zero simultaneously.

[0023] The term c·ITTV provides for a correction especially for high values of ITTV and the term d·p provides for a correction of ITBV especially when the patient is mechanically ventilated. Once the species-specific parameters a, b, c, and d have been determined the application of this formula allows an optimal coincidence between the estimated values of intrathoracic blood volume and extravasal lung water with precisely measured values in a large population of patients.

[0024] In another preferred embodiment of the invention said function $f(GEDV, ITTV, P)$ is selected to be

$$f(GEDV, ITTV, P) = \frac{a}{\frac{(ITTV - GEDV)}{(ITTV_{norm} - GEDV_{norm})} + d \cdot \frac{P}{P_{norm}}} \cdot GEDV + b$$

[0025] a, b, c, and d being species dependent parameters, with $1 < a/(c+d) < 2$, wherein ITTV_{norm}, GEDV_{norm} and P_{norm} are empirical normal values of ITTV, GEDV and P, respectively. Parameters a, b, c, and d are determined by regression.

[0026] In another preferred embodiment of the invention said function $f(GEDV, ITTV, P)$ is selected to be

$$ITBV = \frac{a \cdot GEDV}{\left[c2 \cdot \frac{(ITTV - GEDV)}{(ITTV_{norm} - GEDV_{norm})} + 1 \right] \cdot \left[d2 \cdot \frac{P}{P_{norm}} + 1 \right]} + b + c1 \cdot \frac{(ITTV - GEDV)}{(ITTV_{norm} - GEDV_{norm})} + d1 \cdot \frac{P}{P_{norm}}$$

[0027] parameters a, b, c1, d1, c2, d2 can be obtained by a nonlinear regression from comparative double dilution measurements. The parameters are species dependent. The term $a/(c2+1)(d2+1)$ is normally in the range of 0.5 to 10.

[0028] The first part

$$ITBV = a \cdot GEDV + b + c1 \cdot \frac{(ITTV - GEDV)}{(ITTV_{norm} - GEDV_{norm})} + d1 \cdot \frac{P}{P_{norm}}$$

[0029] describes the total displacement from the thorax to the large circulation.

[0030] The second part

$$ITBV = \frac{a \cdot GEDV}{\left[c2 \cdot \frac{(ITTV - GEDV)}{(ITTV_{norm} - GEDV_{norm})} + 1 \right] \cdot \left[d2 \cdot \frac{P}{P_{norm}} + 1 \right]} + b$$

[0031] describes the changed relation between GEDV and PBV.

[0032] Investigations have shown that with the formula according to the prior art ITBV i.e. the sum of PBV and GEDV was underestimated at high ETV and at high airway pressures. This is because a high ETV leads to a tension of the lung tissue, which is disturbing the normal fixed relation between PBV and GEDV ($ITBV = GEDV + PBV = a \cdot GEDV + b$). A similar result is reached at high airway pressure P.

[0033] Thereby the effective pressure, which is pushing blood out of the lung, is the transmural pressure $P_{tm} = ITP - P_{mv}$. This is the difference between intra thoracic pressure and micro vascular pressure. The peri micro vascular pressure could be neglected. If the lung is very stiff e.g. at a fibrosis, even a high airway pressure has little influence—the intra thoracic pressure remains low.

[0034] Mostly P_{tm} in the micro vessels of the lung is not available. In this case the intra thoracic pressure or the mean airway pressure could be used instead. Because PEEP (positive end expiratory Pressure) is correlated, it could be also useful.

[0035] The blood is displaced from the lung in two ways

[0036] 1. a fraction of the blood is shifted from the lungs into the heart, thereby the normal relation between GEDV and PBV is changed

[0037] 2. a part of the PBV is totally displaced from the thorax to the large circulation (systemic circulation)

[0038] Dependent on the dominant factor $c1$, $d1$ or $c2$, $d2$ could be equal to zero. In a special case of humans $a=1.48$; $b=87\text{ml}$; $c1=-0.18$; $d1=0$; $c2=0$; $d2=0$

[0039] There are also other formulas possible. In general ITBV is a function of GEDV, ITTV and P. It could also be advantageous to apply this to intra thoracic blood volume Index $ITBVI = ITBV/BSA$ which is the ITBV divided by Body surface Area (BSA). In this case ITBVI is a function of GEDV/BSA, TTV/BSA and P.

[0040] In another preferred embodiment of the invention P is set equal to a transmural lung pressure P_{tm} , being defined as $P_{tm} = ITP - P_{mv}$, ITP being a intrathoracic pressure and P_{mv} being a microvascular pressure. As it is the transmural pressure which is responsible for pulmonary vasoconstriction and which is the reason for an overestimation of the intrathoracic blood volume and the underestimation of extravascular lung water best results are obtained by using the transmural pressure for correction of the intrathoracic blood volume, even if the patient suffers from lung fibrosis.

[0041] However, the transmural pressure is sometimes difficult to determine. Fairly good results are also obtained according to another embodiment by using for P a mean pressure measured in the airway of a mechanical respirator

or a positive end expiratory pressure (PEEP) of a mechanical respirator. These pressures can be determined easily.

[0042] Further advantageous embodiments are described in the subclaims.

[0043] The accompanying drawings serve for a better understanding of the above and other features of the present invention.

BRIEF DESCRIPTION OF THE DRAWINGS

[0044] FIG. 1 shows a schematic illustration explaining the dependencies between global end diastolic volume GEDV, pulmonal blood volume PBV, extra thermal volume ETV, airway volume V_{aw} , and airway pressure P.

[0045] FIG. 2 shows a schematic sketch of both a patient's vascular system and a preferred embodiment of an apparatus according to the present invention.

[0046] FIG. 3 shows a schematic example of a Thermodilution Curve in a diagram with the blood temperature difference as a function of time, wherein the abscissa is linear and the ordinate is logarithmic.

[0047] FIG. 4 shows a block diagram illustrating the general hardware structure of an embodiment of a computer system according to the present invention being part of the apparatus sketched in FIG. 2.

DETAILED DESCRIPTION

[0048] FIG. 1 shows a schematic illustration explaining the dependencies between global end diastolic volume GEDV, which is roughly the blood located in the heart, pulmonal blood volume PBV 111, which is the blood located in the lungs, extra thermal volume ETV 112, which is roughly the lung water outside the vessels, air way volume V_{aw} , and air way pressure P. Increasing airway pressure P causes the air way volume V_{aw} to increase, which leads to a decrease of pulmonal blood volume PBV, in other words, the increasing P causes blood to flow out from the lungs into the heart and/or into the systemic circulation. Similarly, increasing ETV also causes blood to flow out from the lungs into the heart and/or into the systemic circulation.

[0049] FIG. 2 illustrates the main components necessary to implement an embodiment of an apparatus according to the invention and schematically shows the first and second places 101, 102 of a patient's vascular system 103, where the apparatus interacts with the patient's vascular system 103. A computer system 104, the general hardware structure of which is schematically illustrated in FIG. 4, is connected via port A 201 with a medical dosage device 105 serving together with a catheter 106 as an injection means 107 to inject at the first place 101, e.g. into patient's vena cava superior, a bolus, e.g. 10 ml, or, as a guideline, 0.15 ml/kg patient's body mass. The bolus serving as a thermal indicator liquid is substantially warmer or colder than patient's blood temperature. As a result, travelling temperature deviation is introduced to the patient's vascular system 103, where it continuously changes according to boundary conditions. The temperature deviation passes right atrium and right ventricle 109 of patient's heart 110 to enter the pulmonary circulation 111, where an extravascular thermovolume 112 may be present in the proximity of the patient's vessels. The temperature deviation passes the left atrium 113

and the left ventricle 114 of patient's heart to enter through the aorta 115 the systemic circulation 116. When the travelling temperature deviation reaches the second place 102, e.g. patient's arteria femoralis, where the patient's blood temperature is continuously measured by a sensor device 117, which is connected to the computer system 104 via port B 202, the travelling temperature deviation is recorded by the computer system 104 as Thermodilution Curve, i.e. temperature measured at the second place 102 as function of time. From this Thermodilution Curve the computer system 104 determines an extravascular thermovolume estimate according to the relations explained above. Extravascular thermovolume correlates, if there is no significant perfusion defect in the lungs (e.g. pulmonary embolism), closely to the degree of Extravascular Lung Water.

[0050] FIG. 4 illustrates the general hardware structure of an embodiment of a computer system 104 according to the invention; suitable to be part of the apparatus shown in FIG. 2. Via ports A and B 201, 202 which belong to an input/output subsystem, the computer system 104 is connectable to injection means 107 sensor device 117 and pressure sensor 118, respectively. The input/output subsystem is controlled by a central processing unit (CPU) 204, which communicates via a data and adress bus 205 with the other components of the computer system 104, which include a timer 206 providing timer clock signals to the CPU 204, a system memory (ROM) 207, in which the system software is permanently stored, a data and instructions memory (RAM) 208, where both executable instructions and various data including temperature readings for thermodilution curves and airway pressure readings can be stored, an input device controller 209 controlling an input device 210, such as a keypad, a touch screen or the like, for manually entering system parameters, operation settings and the like, a disc subsystem 211 to read data or program instructions from a storage medium 212, such as a hard disc, floppy disc, compact disc, optical disc or the like, and to store data to the storage medium 212, and a display subsystem 213 controlling a display 214 to display relevant information, such as a Thermodilution Curve or cardiovascular parameters determined by the computer system 104. The pressure sensor device 118, which is adapted to measure the pressure in patient's airway is connected to the computer system 104 via port 203.

[0051] The above described apparatus is adapted to determine MTT, DST, CO from the thermodilution curve and to calculate parameters such as GEDV, ITBV and ETV.

1. Apparatus for determining intrathoracic blood volume (ITBV) and other cardiovascular parameters of a patient by thermodilution measurements comprising:

- a) temperature influencing means (107) for provoking an initial local temperature change in the proximity of a first place (101) of a patient's vascular system (103), thus introducing a travelling temperature deviation to patient's blood stream,
- b) a temperature sensor device (117) for measuring the local temperature of patient's blood at a second place (102) of patient's vascular system (103) downstream of said first place (101)
- c) a computer system (104) coupled to said temperature sensor device (117) and adapted to record said patient's

local blood temperature measured at said second place (102) as a function of time to determine a thermodilution curve,

- d) said computer system (104) being further adapted to determine patient's global enddiastolic blood volume (GEDV) and patient's intrathoracic thermovolume (ITTV) from said thermodilution curve,
- e) said computer system (104) being further adapted to determine patient's intrathoracic blood volume (ITBV) according to the following formula:

$$ITBV=f(GEDV, ITTV, P),$$

ITBV being the intrathoracic blood volume, GEDV being the global enddiastolic blood volume, ITTV being the intrathoracic thermovolume, P being an airway pressure inside patient's lungs.

2. Apparatus as claimed in claim 1, wherein said function f(GEDV, ITTV, P) is selected to be

$$f(GEDV, ITTV, P)=a \cdot GEDV+b+c \cdot ITTV+d \cdot P$$

- a being a species dependent parameter, with $1 < a < 2$
- b being a species dependent parameter, including zero
- c being a species dependent parameter, with $c \leq 0$
- d being a species dependent parameter, including zero, with the restriction that c and d may not be zero simultaneously.

3. Apparatus as claimed in claim 1, wherein said function f(GEDV, ITTV, P) is selected to be

$$f(GEDV, ITTV, P) = \frac{a}{\frac{(ITTV - GEDV)}{(ITTV_{norm} - GEDV_{norm})} + d \cdot \frac{P}{P_{norm}}} \cdot GEDV + b$$

- a, b, c, and d being species dependent parameters, with $1 < a/(c+d) < 2$, wherein ITTVnorm, GEDVnorm and Pnorm are empirical normal values of ITTV, GEDV and P, respectively.

4. Apparatus as claimed in claim 1, wherein said function f(G EDV, ITTV, P) is selected to be

$$ITBV = \frac{a \cdot GEDV}{\left[c^2 \cdot \frac{(ITTV - GEDV)}{(ITTV_{norm} - GEDV_{norm})} + 1 \right] \cdot \left[d^2 \cdot \frac{P}{P_{norm}} + 1 \right]} + b + c1 \cdot \frac{(ITTV - GEDV)}{(ITTV_{norm} - GEDV_{norm})} + d1 \cdot \frac{P}{P_{norm}}$$

- a, b, c1, c2, d1, d2 being species dependent parameters, with $0,5 \leq a/(c2+1)(d2+1) \leq 10$, wherein ITTVnorm, GEDVnorm and Pnorm are empirical normal values of ITTV, GEDV and P, respectively.

5. Apparatus as claimed in claim 1 wherein P is set equal to a transmural lung pressure Ptm, being defined as

$$P_{tm}=ITP-P_{mv};$$

ITP being a intrathoracic pressure and Pmv being a microvascular pressure.

6. Apparatus as claimed in claim 1, wherein P is a pressure measured in the airway of a mechanical respirator.

7. Apparatus as claimed in claim 6, wherein P is a positive end expiratory pressure (PEEP).

8. Apparatus as claimed in claim 1, wherein P is a mean airway pressure.

9. Apparatus as claimed in claim 1 which is adapted to determine at least one of said cardio-vascular parameters by transpulmonary thermodilution.

10. Apparatus as claimed in claim 1 which is adapted to determine an estimate of extravascular lung water (EVLW) as

$$EVLW=ITTV-ITBV,$$

EVLW being the extravascular lung water.

11. Apparatus as claimed in claim 1 which is adapted to determine ITTV as

$$ITTV=CO \cdot MTT,$$

CO being the cardiac output and MTT being the mean transit time, indicating the time required by said temperature deviation to travel from said first place (101) to said second place (102).

12. Apparatus as claimed in claim 1 which is adapted to determine GEDV as

$$GEDV=CO \cdot (MTT-DST),$$

CO being the cardiac output and MTT being the mean transit time, indicating the time required by said temperature deviation to travel from said first place (101) to said second place (102) and DST being a down slope time of said thermodilution curve.

13. Apparatus as claimed in claim 1 further comprising a pressure sensing device (118) coupled to said computer system (104).

14. Computer system (104) comprising first coupling means to couple said computer system (104) to temperature influencing means (107) and second coupling means to couple said computer system (104) to a temperature sensor device (117), and accessing means to access executable instructions to cause said computer system (104)

a) to control temperature influencing means (107) for provoking an initial local temperature change in the proximity of a first place (101) of a patient's vascular system (103), thus introducing a travelling temperature deviation to patient's blood stream,

b) to record said patient's local blood temperature measured by a temperature sensor device (117) for measuring the local temperature of patient's blood at a second place (102) of patient's vascular system (103) downstream of said first place (101) as a function of time to determine a thermodilution curve,

c) to determine patient's global enddiastolic blood volume (GEDV) and patient's intrathoracic thermovolume (ITTV) from said thermodilution curve,

e) to determine patient's intrathoracic blood volume (ITBV) according to the following formula:

$$ITBV=f(GEDV, ITTV, P),$$

ITBV being the intrathoracic blood volume, GEDV being the global enddiastolic blood volume, ITTV being the intrathoracic thermovolume, P being an airway pressure inside patient's lungs.

15. Computer system as claimed in claim 14, wherein said function $f(GEDV, ITTV, P)$ is selected to be

$$f(GEDV, ITTV, P)=a \cdot GEDV+b+c \cdot ITTV+d \cdot P$$

a being a species dependent parameter, with $1 < a < 2$

b being a species dependent parameter, including zero

c being a species dependent parameter, with $c \leq 0$

d being a species dependent parameter, including zero, with the restriction that c and d may not be zero simultaneously.

16. Computer system as claimed in claim 14, said function $f(GEDV, ITTV, P)$ is selected to be

$$f(GEDV, ITTV, P) = \frac{a}{\frac{(ITTV - GEDV)}{c \cdot (ITTV_{norm} - GEDV_{norm})} + d \cdot \frac{P}{P_{norm}}} \cdot GEDV + b$$

a, b, c, and d being species dependent parameters, with $1 < a/(c+d) < 2$, wherein ITTVnorm, GEDVnorm and Pnorm are empirical normal values of ITTV, GEDV and P, respectively.

17. Computer system as claimed in claim 14, wherein said function $f(GEDV, ITTV, P)$ is selected to be

$$ITBV = \frac{a \cdot GEDV}{\left[c2 \cdot \frac{(ITTV - GEDV)}{(ITTV_{norm} - GEDV_{norm})} + 1 \right] \cdot \left[d2 \cdot \frac{P}{P_{norm}} + 1 \right]} + b + c1 \cdot \frac{(ITTV - GEDV)}{(ITTV_{norm} - GEDV_{norm})} + d1 \cdot \frac{P}{P_{norm}}$$

a, b, c1, c2, d1, d2 being species dependent parameters, with $0,5 \leq a/(c2+1)(d2+1) \leq 10$, wherein ITTVnorm, GEDVnorm and Pnorm are empirical normal values of ITTV, GEDV and P, respectively.

18. Computer system as claimed in claim 1, comprising a port coupled to a pressure sensor arranged in the airway of a mechanical respirator.

19. Computer system as claimed in claim 1 being caused to determine an estimate of extravascular lung water (EVLW) as

$$EVLW=ITTV-ITBV,$$

EVLW being the extravascular lung water.

20. Computer system as claimed in claim 1 being caused to determine said ITTV as

$$ITTV=CO \cdot MTT,$$

CO being the cardiac output and MTT being the mean transit time, indicating the time required by said temperature deviation to travel from said first place (101) to said second place (102).

21. Computer system as claimed in claim 1 being caused to determine said GEDV as

$$GEDV=CO \cdot (MTT-DST),$$

CO being the cardiac output and MTT being the mean transit time, indicating the time required by said temperature deviation to travel from said first place (101)

to said second place (102) and DST being a down slope time of said thermodilution curve.

22. Computer program for determining intrathoracic blood volume (ITBV) and other cardio-vascular parameters of a patient by thermodilution measurements comprising instructions executable by a computer system (104) to cause said computer system (104)

- a) to control temperature influencing means (107) for provoking an initial local temperature change in the proximity of a first place (101) of a patient's vascular system (103), thus introducing a travelling temperature deviation to patient's blood stream,
- b) to record said patient's local blood temperature measured by a temperature sensor device (117) for measuring the local temperature of patient's blood at a second place (102) of patient's vascular system (103) downstream of said first place (101) as a function of time to determine a thermodilution curve,
- c) to determine patient's global enddiastolic blood volume (GEDV) and patient's intrathoracic thermovolume (ITTV) from said thermodilution curve,
- e) to determine patient's intrathoracic blood volume (ITBV) according to the following formula:

$$ITBV=f(GEDV, ITTV, P),$$

ITBV being the intrathoracic blood volume, GEDV being the global enddiastolic blood volume, ITTV being the intrathoracic thermovolume, P being an airway pressure inside patient's lungs.

23. Computer program as claimed in claim 22, wherein said function f(GEDV, ITTV, P) is selected to be

$$f(GEDV, ITTV, P)=a \cdot GEDV+b+c \cdot ITTV+d \cdot P$$

- a being a species dependent parameter, with $1 < a < 2$
 - b being a species dependent parameter, including zero
 - c being a species dependent parameter, with $c \leq 0$
 - d being a species dependent parameter, including zero,
- with the restriction that c and d may not be zero simultaneously.

24. Computer program as claimed in claim 22, said function f(GEDV, ITTV, P) is selected to be

$$f(GEDV, ITTV, P) = \frac{a}{\frac{(ITTV - GEDV)}{ITTV_{norm} - GEDV_{norm}} + d \frac{P}{P_{norm}}} \cdot GEDV + b$$

a, b, c, and d being species dependent parameters, with $1 < a/(c+d) < 2$, wherein ITTVnorm, GEDVnorm and Pnorm are empirical normal values of ITTV, GEDV and P, respectively.

25. Computer program as claimed in claim 22, wherein said function f(GEDV, ITTV, P) is selected to be [Fließendes Objekt]

a, b, c1, c2, d1, d2 being species dependent parameters, with $0,5 \leq a/(c2+1)(d2+1) \leq 10$, wherein ITTVnorm, GEDVnorm and Pnorm are empirical normal values of ITTV, GEDV and P, respectively.

26. Computer program as claimed in claim 1 causing said computer system (104) to determine an estimate of extravascular lung water (EVLW) as

$$EVLW=ITTV-ITBV,$$

EVLW being the extravascular lung water.

27. Computer program as claimed in claim 1 causing said computer system (104) to determine ITTV as

$$ITTV=CO \cdot MTT,$$

CO being the cardiac output and MTT being the mean transit time, indicating the time required by said temperature deviation to travel from said first place (101) to said second place (102).

28. Computer program as claimed in claim 1 causing said computer system (104) to determine GEDV as

$$GEDV=CO \cdot (MTT-DST),$$

CO being the cardiac output and MTT being the mean transit time, indicating the time required by said temperature deviation to travel from said first place (101) to said second place (102) and DST being a down slope time of said thermodilution curve.

29. Storage medium (212) having physically stored thereon a computer program as claimed in claim 1.

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专利名称(译)	用于确定胸内血容量和其他心血管参数的装置，计算机系统和计算机程序		
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摘要(译)

用于通过热稀释测量确定患者的胸内血容量 (ITBV) 和其他心血管参数的装置，计算机系统，计算机程序和存储介质。该装置包括a) 温度影响装置 (107)，用于在患者血管系统 (103) 的第一位置 (101) 附近引起初始局部温度变化，从而引入患者血流的行进温度偏差，b) 温度传感器装置 (117)，用于在所述第一位置 (101) 下游的患者血管系统 (103) 的第二位置 (102) 测量患者血液的局部温度c) 连接到所述温度传感器的计算机系统 (104) 设备 (117) 并且适于记录在所述第二位置 (102) 测量的所述患者的局部血液温度作为时间的函数以确定热稀释曲线，d) 所述计算机系统 (104) 还适于确定患者的全球舒张末期血容量来自所述热稀释曲线的 (GEDV) 和患者的胸内热量 (ITTV) e) 所述计算机系统 (104) 还适于确定患者的胸内血容量 (ITBV)。ng到以下公式： $ITBV = f(GEDV, ITTV, P)$ ，ITBV是胸内血容量，GEDV是全球舒张末期血容量，ITTV是胸内热容量，P是患者肺部内的气道压力。通过确定ITBV不仅来自GEDV而且还作为ITTV和P的函数，可以获得增强的准确性，特别是如果患者患有肺水肿和/或机械通气。

