



US 20040220499A1

(19) **United States**

(12) **Patent Application Publication** (10) **Pub. No.: US 2004/0220499 A1**
Griego et al. (43) **Pub. Date: Nov. 4, 2004**

(54) **MEDICAL INSTRUMENT WITH CONTROLLED TORQUE TRANSMISSION**

(52) **U.S. Cl. 600/585; 29/592; 140/71 R**

(75) **Inventors: John A. Griego, Blackstone, MA (US); Patrice A. Weststrate, Norwood, MA (US)**

(57) **ABSTRACT**

Correspondence Address:
CHRISTENSEN, O'CONNOR, JOHNSON, KINDNESS, PLLC
1420 FIFTH AVENUE
SUITE 2800
SEATTLE, WA 98101-2347 (US)

A medical instrument such as a guidewire that is designed to have controlled torque transmission along its length. Specially treated areas are placed in selected and equal areas along the entire length of the elongated shaft of the medical instrument, and are separated from one another by untreated areas. This process ensures that any torque is transmitted distally, in a smooth manner, regardless of the guidewire position, thus resulting in a substantial reduction in whipping. In one embodiment, a stainless steel guidewire is utilized, and is subjected to annealing heat treatment in selected areas. This annealing process creates a mandrel that has repeated temper properties along its length. Torque applied at one end of this mandrel is transmitted to the opposite end in an even and controlled manner, even when the mandrel is formed into a loop.

(73) **Assignee: Scimed Life Systems, Inc.**

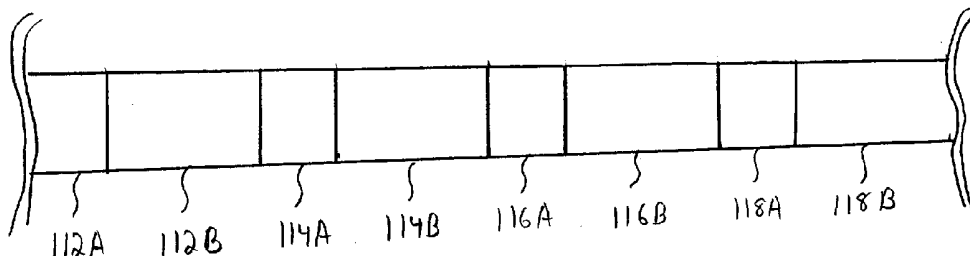
(21) **Appl. No.: 10/428,240**

(22) **Filed: May 1, 2003**

Publication Classification

(51) **Int. Cl.⁷ A61B 5/00**

100
↓



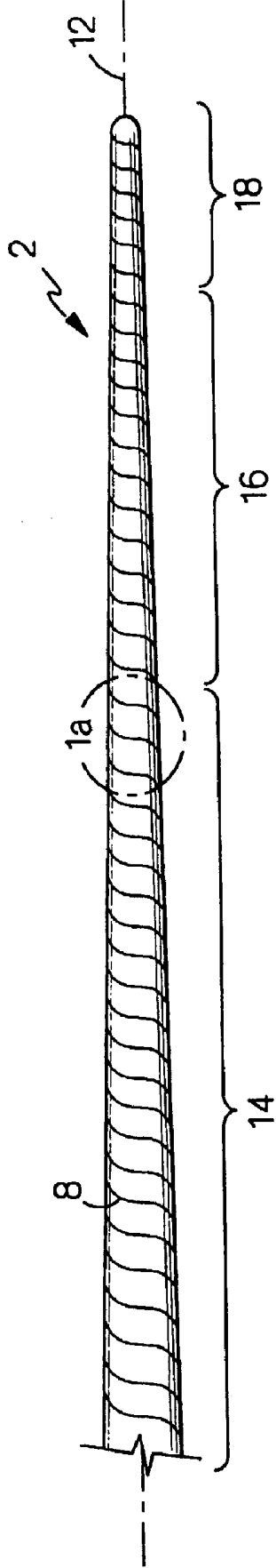


Fig. 1.
(prior art)

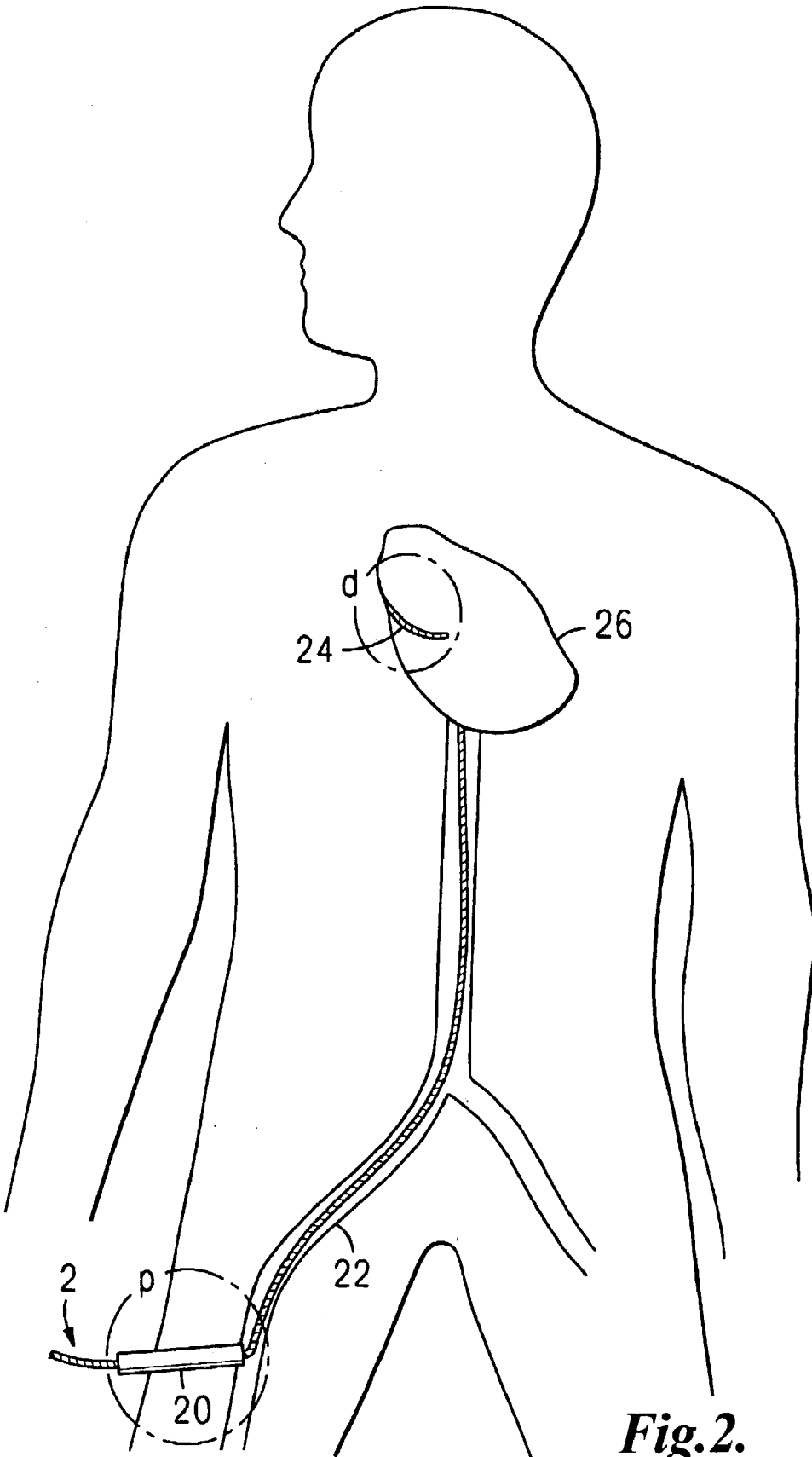


Fig.2.
(prior art)

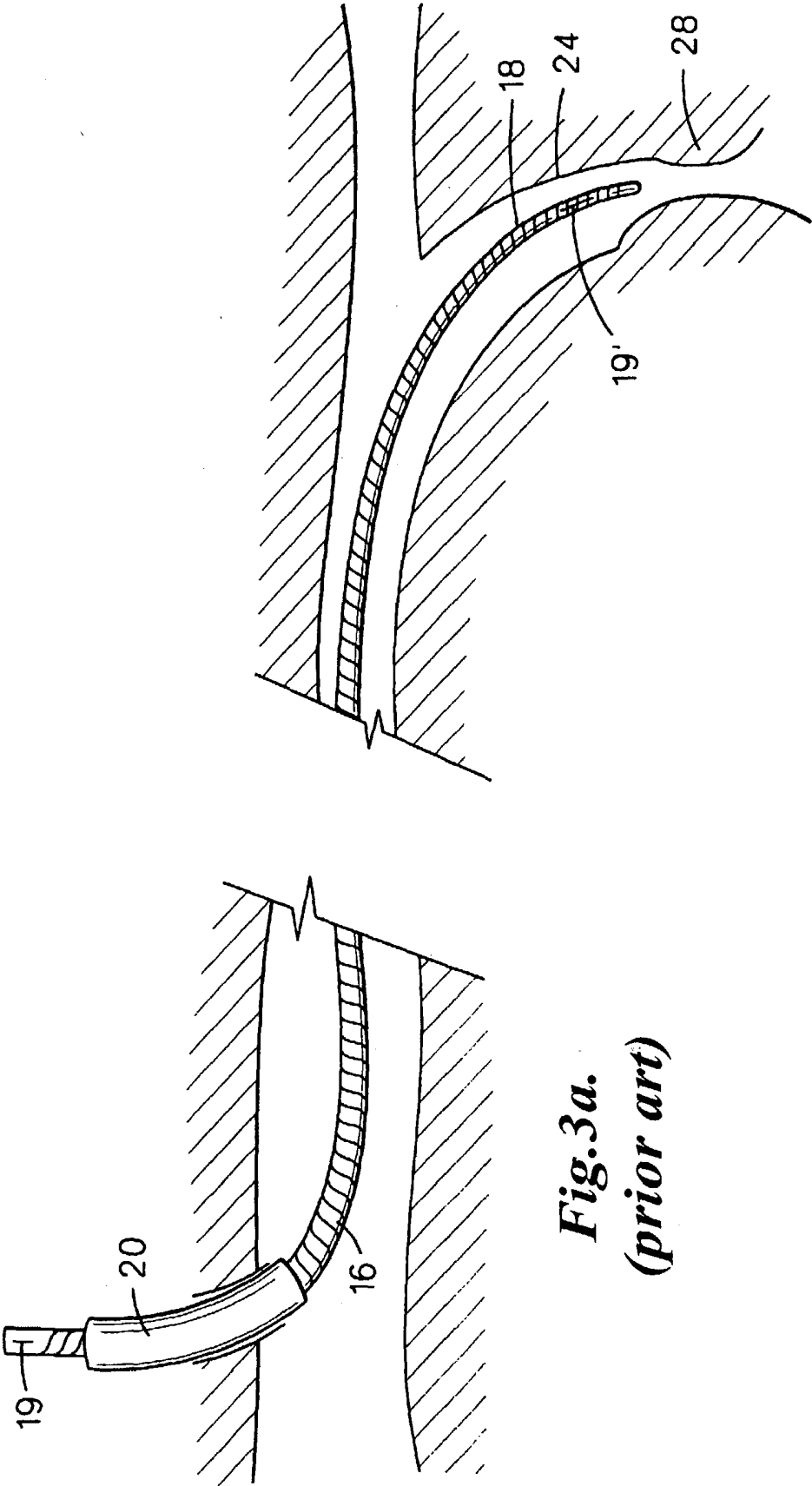


Fig. 3a.
(prior art)

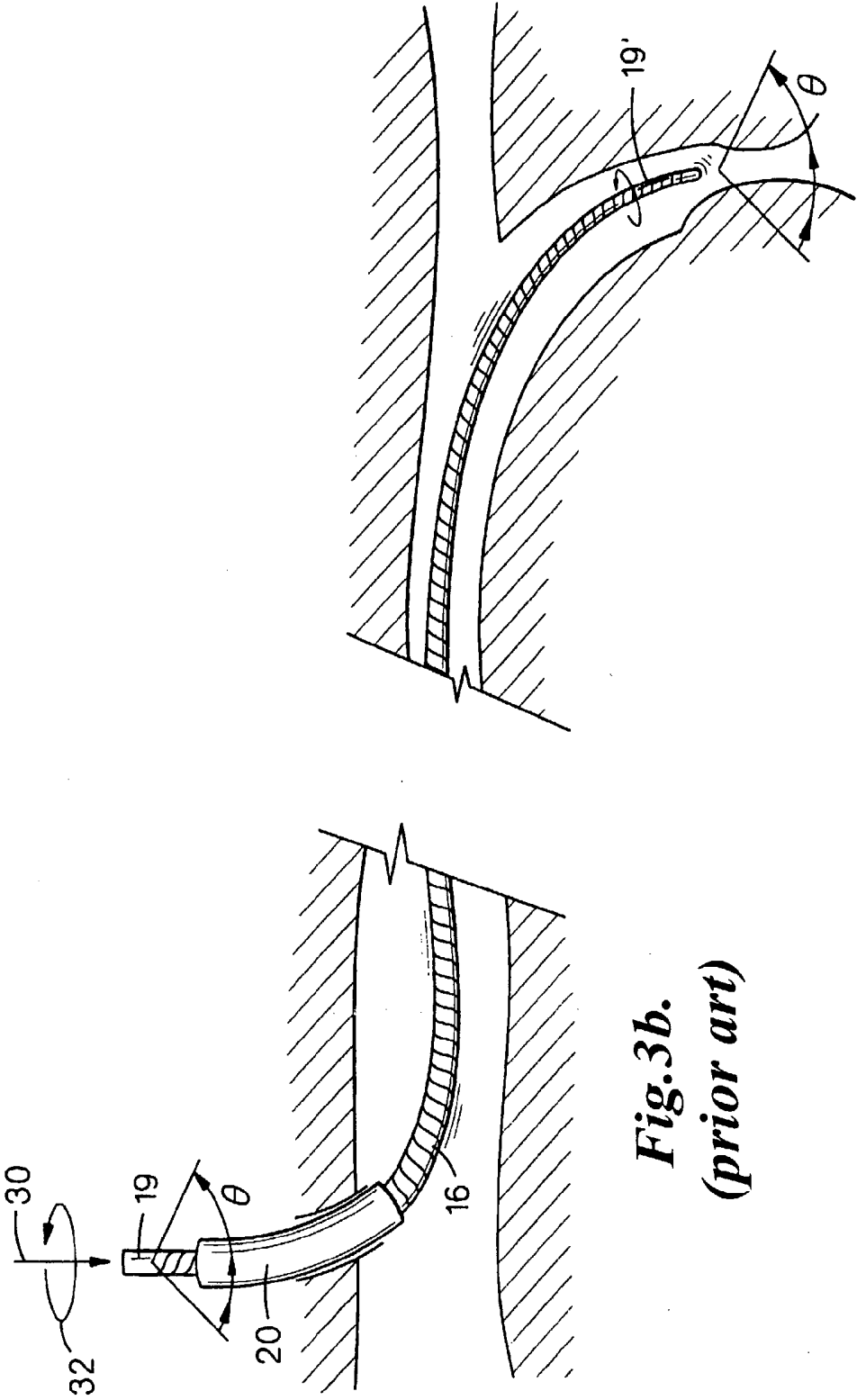


Fig. 3b.
(prior art)

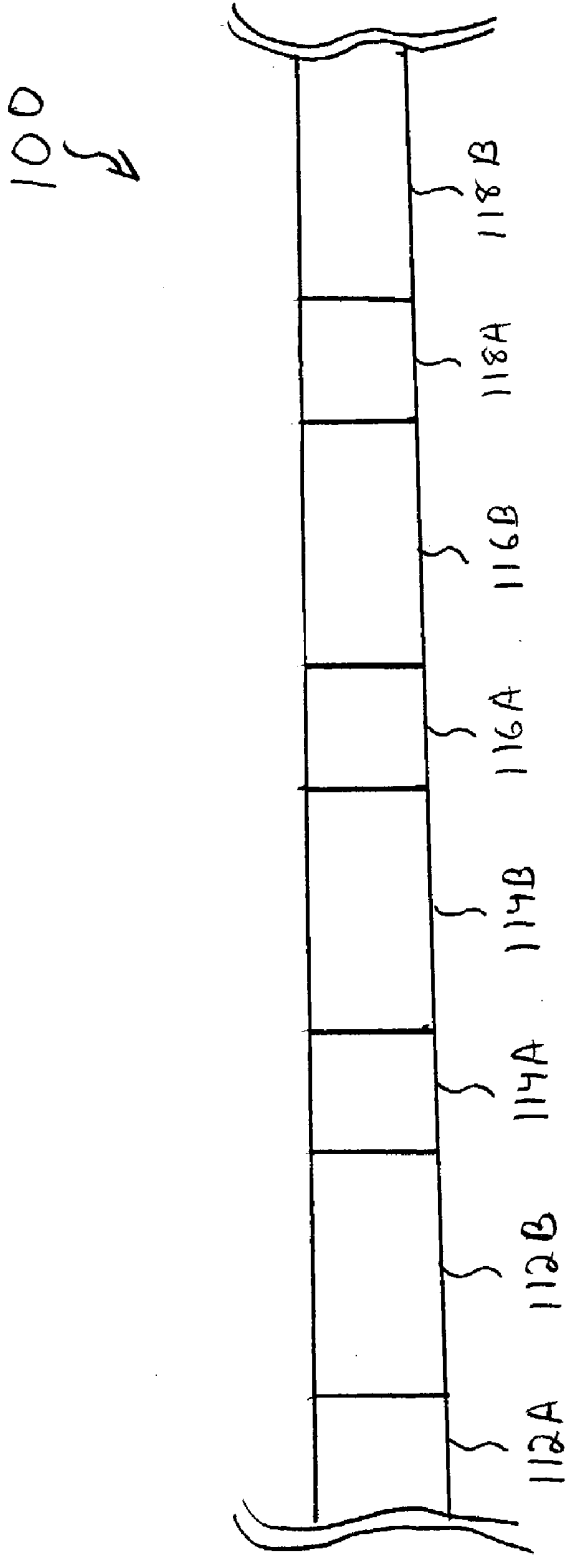


Fig. 4.

MEDICAL INSTRUMENT WITH CONTROLLED TORQUE TRANSMISSION

FIELD OF THE INVENTION

[0001] The invention relates to medical instruments such as guidewires, and more particularly to a medical instrument such as a guidewire that is designed to have controlled torque transmission along its length.

BACKGROUND OF THE INVENTION

[0002] Guidewires are used in most catheter-based procedures. The distal end of a guidewire typically has an angled tip, which can be oriented to help steer the guidewire through curves and junctions of the vasculature or vessels of a patient. The orientation of the angled tip is achieved by torquing the guidewire so that it rotates about its axis.

[0003] Correct positioning of a catheter is dependent on the ability of the guidewire to track and be rotated to gain access to the target area. Guidewires generally will rotate in a 1:1 ratio between the proximal and distal ends in a straightened position, however, when subject to looping or bending as may occur in a tortuous anatomy, guidewires exhibit the tendency to whip (sudden release of torsional energy). This whipping makes precise access to target sites, such as selecting one vessel of a bifurcation, difficult.

[0004] Often, because of the variability of procedures and anatomy, the location of the hoop stress created by looping or bending of the guidewire cannot be predicted. Guidewires that are produced by maintaining a rigid proximal end and sequentially creating a more flexible distal portion are subject to whipping when looping or bending is applied away from the end of the distal portion.

[0005] One prior art device and method for torque transmission in a guidewire is shown in U.S. Pat. No. RE 36,628, to Sagae et al. The '628 patent teaches a catheter guidewire wherein the base material constituting the wire is made of an elastic alloy wire and is subjected to a heat treatment such that its flexibility is sequentially increased from its proximal to distal end portions. A thermoplastic resin and/or a coil spring may be applied to at least the distal end portion of the wire base material. A method of manufacturing the catheter guidewire is also taught. The method is characterized in that the leading end side of the base material is divided into a plurality of areas and subjected to a heat treatment by changing the heat treatment temperature and the time conditions in units of the areas so that the flexibility of the base material is sequentially increased from the proximal to distal end portions of the leading end side. As noted above, one of the drawbacks of guidewires such as that taught in the '628 patent is that guidewires that are produced by maintaining a rigid proximal end and sequentially creating a more flexible distal portion are subject to whipping when looping or bending is applied away from the end of the distal portion.

[0006] Another prior art device and method for torque transmission is taught in U.S. Pat. No. 5,951,494, which is hereby incorporated by reference. FIGS. 1-3 herein have been reproduced from the '494 patent. Referring to FIG. 1, a guidewire 2 includes a relatively stiff proximal portion 14, a transition portion 16 with varying, intermediate stiffness, and a highly flexible distal portion 18. The guidewire is formed entirely of common medical polymer materials and

exhibits high torque fidelity because it has been twisted and tensioned in manufacture to helically orient the polymer. This is illustrated by a segment 8 of the wire that, prior to processing, was parallel to the device axis but after twisting and tensioning, follows a characteristic helical path.

[0007] Referring to FIG. 2, in the course of an angioplasty operation to open an occluded coronary artery, the guidewire 2 is typically delivered through an access catheter 20 into the femoral artery 22. The physician pushes and torques the proximal end of the guidewire to thread it through the body into the coronary arteries 24.

[0008] Referring to FIGS. 3A and 3B, the distal portion 18 of the guidewire is positioned such that it can cross a restricted region 28 of the artery. The physician pushes (arrow 30) and torques (arrow 32) the proximal portion of the guidewire remaining outside the body. The degree of rotation caused by torquing the proximal end is transmitted to produce a degree of rotation at the distal end.

[0009] As noted above, guidewires that are produced by maintaining a rigid proximal end and sequentially creating a more flexible distal portion are subject to whipping when looping or bending is applied away from the end of the distal portion. In addition, guidewires that are formed from certain elastic alloys are relatively expensive to produce. The present invention is directed to a device and method for overcoming the foregoing and other disadvantages. More specifically, the present invention is directed to a medical instrument such as a guidewire that is designed to have controlled torque transmission along its length.

SUMMARY OF THE INVENTION

[0010] In accordance with the present invention, a medical instrument such as a guidewire is provided that can be rotated without whipping. In addition to guidewires, other applications include devices such as catheters and drive-shafts. In one embodiment, the medical instrument tapers at the distal portion to promote access to anatomy that reduces in inner diameter.

[0011] In accordance with another aspect of the invention, specially treated areas are placed in selected and equal areas along the entire length of the elongated shaft of the medical instrument, and are separated from one another by untreated areas. This process ensures that any torque is transmitted distally, in a smooth manner, regardless of the guidewire position, thus resulting in a substantial reduction in whipping. In one embodiment, a stainless steel guidewire is utilized, and is subjected to annealing heat treatment in selected areas. This annealing process will create a mandrel that has repeated temper properties along its length. Torque applied at one end of this mandrel is transmitted to the opposite end in an even and controlled manner, even when the mandrel is formed into a loop.

[0012] In accordance with another aspect of the invention, the treated sections are subjected to an annealing process, while the untreated sections are normally tempered. The untreated sections may be longer than the treated sections. In one embodiment, the treated sections are all approximately the same length.

BRIEF DESCRIPTION OF THE DRAWINGS

[0013] The foregoing aspects and many of the attendant advantages of this invention will become more readily

appreciated as the same become better understood by reference to the following detailed description, when taken in conjunction with the accompanying drawings, wherein:

[0014] FIG. 1 is a side view of a prior art polymer medical guidewire;

[0015] FIG. 2 is a schematic of the prior art guidewire of FIG. 1, as being delivered into a patient;

[0016] FIGS. 3A and 3B are expanded views of the prior art guidewire of FIG. 2 illustrating torquing of the proximal end and rotation of the distal end; and

[0017] FIG. 4 is a side view of a guidewire that has been subjected to heat treatments in selected areas in accordance with the present invention.

DETAILED DESCRIPTION OF THE PREFERRED EMBODIMENT

[0018] Low carbon alloy steel, such as stainless steel, has strength and hardness imparted through drawing or extrusion. This hardness is an ideal quality for guidewires as they can be torqued effectively over a long length. A guidewire made from this material is very cost effective as compared to a wire made from elastic alloys such as nitinol. An important factor is the ability of the wire to track and thus create a mechanical pathway through a portion of the human anatomy in order to allow a physician to direct other devices such as catheters to a precise location.

[0019] The ability to track is related to a combination of both pushing and rotating the guidewire. Often placed in a tortuous path, a guidewire cannot effectively transmit torque from the proximal to the distal end in a 1:1 ratio. As the proximal end is rotated, the torsion is stored as energy in the end of the guidewire proximal to the tortuous path. When the threshold is reached where the stored energy overcomes the resistance of the tortuous path, whipping of the distal tip of the guidewire will occur. As a result, accurate placement of the guidewire is difficult.

[0020] FIG. 4 is a side view of a guidewire 100 that is formed in accordance with the present invention. The guidewire 100 has been subjected to selective area annealing. More specifically, localized sections 112a, 114a, 116a, and 118a have been subjected to selected area annealing. The sections 112b, 114b, 116b, and 118b are untreated (normally tempered) sections.

[0021] As noted above, the use of stainless steel as the material is a cost-effective choice for the guidewire 100. In one embodiment, the guidewire 100 comprises an elongated stainless steel element with a length of 220 cm and an outer diameter of 0.018 inches. The stainless steel guidewire 100 is provided with a tapered distal tip. The taper, as in most guidewires, increases the flexibility at the distal end. To improve the ability to push the guidewire 100, the middle and proximal sections are greater in diameter than the distal end. As described above, the middle section may be severely turned as it passes through the aortic arch into the carotid arteries. A curve in the guidewire 100 would be an area where effective torque transmission could be hampered, and which could cause the distal tip to whip upon attempted rotation of the guidewire 100. In this instance, a more ductile middle section that is formed in accordance with the present invention will aid in torque transmission without whipping.

[0022] As an example embodiment, in an experiment a guidewire 100 was formed by creating a repeating pattern of 1 cm heat treated (annealed) sections (e.g., 112a, 114a, 116a, 118a) followed by 2 cm untreated (normally tempered) sections (e.g., 112b, 114b, 116b, 118b). These sections were produced working 20 cm from the proximal end of a 150 cm long, 0.16" diameter stainless steel shaft guidewire 100. In the experiment, to form the guidewire 100 a hydrogen gas generator was fitted with a torch tip that produced a flame 0.030" in diameter and approximately 0.200" long. The annealing temperature for stainless steel is approximately 1200 degrees Fahrenheit. In the experiment, the stainless steel was heated with the hydrogen gas torch until it just changed from a dark red color to a bright red color. In order to create very localized sections, a short annealing time was applied to the 1 cm sections (e.g., 112a, 114a, 116a, 118a). The short annealing time comprised raising each of the sections from room temperature to above 1,280 degrees Fahrenheit over approximately 10 seconds. Heat sinks were used to protect the untreated sections (e.g., 112b, 114b, 116b, 118b). Time as well as heat is important for proper annealing so the heat was allowed to rise above the 1280 degree Fahrenheit mark briefly to compensate for time. The process was followed by a quick quench. Once the guidewire 100 was formed according to this process, it was tested in a looped environment and there was a substantial reduction in whipping for the guidewire 100 as compared with an untreated guidewire of the same material. In other words, upon rotation at the proximal end, a substantial reduction in whipping at the distal end was apparent for the guidewire 100 as compared to an untreated guidewire of the same material.

[0023] In actual production, in one embodiment a guidewire 100 may be produced by utilizing RF generation and induction coil heating to achieve selective annealing. Induction heating at precise local areas and for a specific time restores ductility to the heat-treated areas while the hardness of the untreated areas is not compromised. An automated system may be used to control atmosphere, movement, temperature, duration and post process actions such as quenching.

[0024] While the preferred embodiment of the invention has been illustrated and described, it will be appreciated that various changes can be made therein without departing from the spirit and scope of the invention. For example, the guidewire may be further coated with materials such as silicone or hydrophilic coatings. In addition, a coiled platinum spring may be provided at the distal end to aid in the flexibility. The guidewire may comprise either a tapered wire from the proximal end to the distal tip, or a straight wire from the proximal end to the distal tip, or any combination thereof. Furthermore, a stainless steel wire base tensile strength can be varied to fit applications where more or less flexibility is required. In addition, a guidewire torque device may be provided to assist with the rotation of the guidewire. Many types of guidewires may benefit from the disclosed method of production, such as neuro/coronary/peripheral vascular guidewires. Other applications include devices such as catheters and driveshafts, as well as other instruments that use shafts which require rotation, such as retrieval baskets and snares. The selective annealing procedure may also aid in the flexibility of devices such as stents, where variable stiffness could aid placement in tortuous anatomy.

Various types of metals and materials may be utilized, being either round or non-round, that can be subjected to annealing or tempering.

The embodiments of the invention in which an exclusive property or privilege is claimed are defined as follows:

1. An elongated medical instrument that is subject to torque when in use, comprising:

a first plurality of sections that have been subjected to a selected treatment process;

a second plurality of sections located between each of the sections of the first plurality of sections, the second plurality of sections not having been subjected to the selected treatment process; and

wherein the first plurality of sections and the second plurality of sections have different torque transmission characteristics.

2. The medical instrument of claim 1, wherein the selected treatment process is a heat treatment process.

3. The medical instrument of claim 2, wherein the heat treatment process is an annealing process.

4. The medical instrument of claim 3, wherein the second plurality of sections are normally tempered.

5. The medical instrument of claim 1, wherein each of the sections in the first plurality of sections are approximately the same length.

6. The medical instrument of claim 5, wherein each of the sections in the second plurality of sections are approximately the same length.

7. The medical instrument of claim 6, wherein each of the sections in the second plurality of sections is approximately twice as long as the sections in the first plurality of sections.

8. The medical instrument of claim 1, wherein the medical instrument comprises stainless steel.

9. The medical instrument of claim 1, wherein the medical instrument is tapered along at least part of its length.

10. The medical instrument of claim 1, wherein the medical instrument is a guidewire.

11. An elongated medical instrument comprising an elongated structural body, the body having repeated temper

properties along its length, the repeated temper properties including annealed properties interspersed with normally tempered properties.

12. The medical instrument of claim 11, wherein the annealed properties are contained in sections of the structural body that are separated by sections having the normally tempered properties.

13. The medical instrument of claim 11, wherein the structural body is tapered along at least part of its length.

14. The medical instrument of claim 11, wherein the sections of the structural body that have the normally tempered properties are at least as long as the sections of the body that have the annealed properties.

15. A method for treating an elongated medical instrument, comprising:

preparing a heating process for heating a plurality of selected sections of the medical instrument; and

subjecting the plurality of selected sections of the medical instrument to the heating process so as to alter the torque characteristics of the plurality of selected sections, the plurality of selected sections of the medical instrument being separated from one another by a plurality of unselected sections that are not subjected to the heating process.

16. The method of claim 15, wherein the medical instrument is formed of stainless steel and the heating process raises the temperature of the plurality of selected sections above approximately 1200° F.

17. The method of claim 15, wherein the plurality of unselected sections that are not subjected to the heating process are protected from the heating process.

18. The method of claim 17, wherein the plurality of unselected sections are protected from the heating process by heat sinks.

19. The method of claim 15, wherein the heating process is followed by a quick quench process.

20. The method of claim 15, wherein each of the sections in the plurality of selected sections is approximately the same length.

* * * * *

专利名称(译)	具有受控扭矩传递的医疗仪器		
公开(公告)号	US20040220499A1	公开(公告)日	2004-11-04
申请号	US10/428240	申请日	2003-05-01
申请(专利权)人(译)	SCIMED LIFE SYSTEMS INC.		
当前申请(专利权)人(译)	BOSTON SCIENTIFIC SCIMED , INC.		
[标]发明人	GRIEGO JOHN A WESTSTRATE PATRICE A		
发明人	GRIEGO, JOHN A. WESTSTRATE, PATRICE A.		
IPC分类号	A61B5/00 A61M25/00 A61M25/01 A61M25/16		
CPC分类号	A61M25/09 A61M2025/09108 Y10T29/49 A61M2025/09175 A61M25/09033		
其他公开文献	US7780611		
外部链接	Espacenet USPTO		

摘要(译)

一种医疗器械，例如导丝，其设计成沿其长度具有受控的扭矩传递。经特殊处理的区域沿着医疗器械的细长轴的整个长度放置在选定的和相等的区域中，并且通过未处理的区域彼此分开。该过程确保无论导丝位置如何都以平滑的方式向远侧传递任何扭矩，从而导致搅打的显著减少。在一个实施例中，使用不锈钢导丝，并在选定区域进行退火热处理。该退火过程产生了沿其长度具有重复回火特性的心轴。在该心轴的一端施加的扭矩以均匀且受控的方式传递到相对端，即使心轴形成环。

