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(54) **SYSTEMS AND METHODS FOR INCREASED SPECIFICITY IN DIAGNOSTICS**

USPC 607/9, 25–26, 17–18, 62; 600/516, 600/508–509, 513

See application file for complete search history.

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A61B 5/0452 (2006.01)
A61B 5/00 (2006.01)
A61N 1/365 (2006.01)

(52) **U.S. Cl.**

CPC **A61B 5/0452** (2013.01); **A61B 5/4842** (2013.01); **A61N 1/365** (2013.01); **A61B 5/686** (2013.01)
USPC **600/509**

(58) **Field of Classification Search**

CPC **A61B 5/0452**; **A61B 5/686**; **A61B 5/4842**;
A61N 1/365

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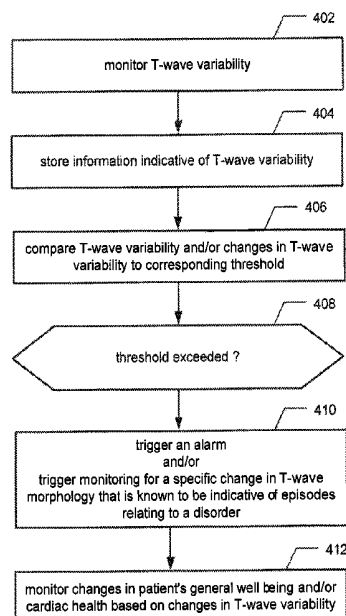
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(57) **ABSTRACT**

Methods and apparatuses for monitoring, with improved specificity, occurrences of episodes relating to disorders that are known to affect T-wave morphology. T-wave variability is monitored. When T-wave variability, or a change therein, exceeds a corresponding threshold for a specific period of time, monitoring for a specific change in T-wave morphology that is known to be indicative of episodes relating to a disorder may be triggered.

20 Claims, 9 Drawing Sheets



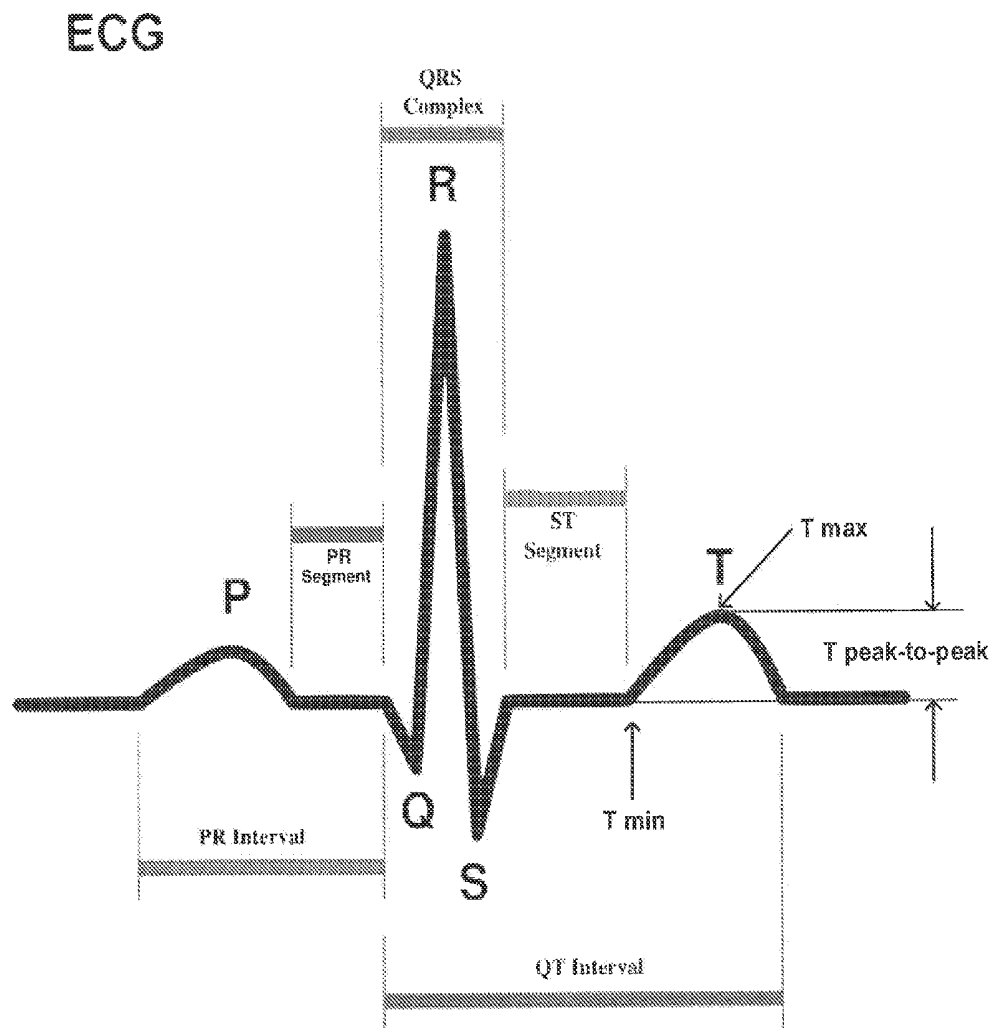


FIG. 1A

IEGMs

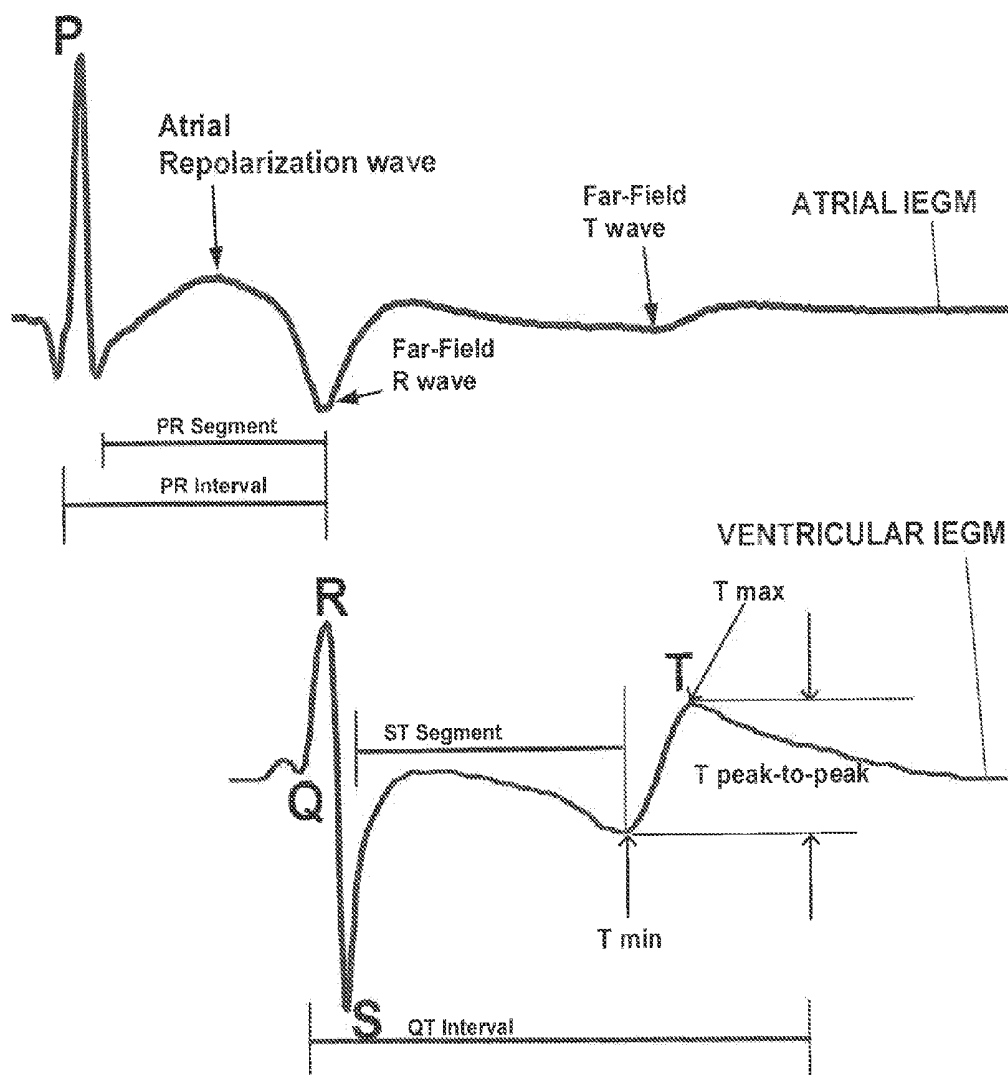
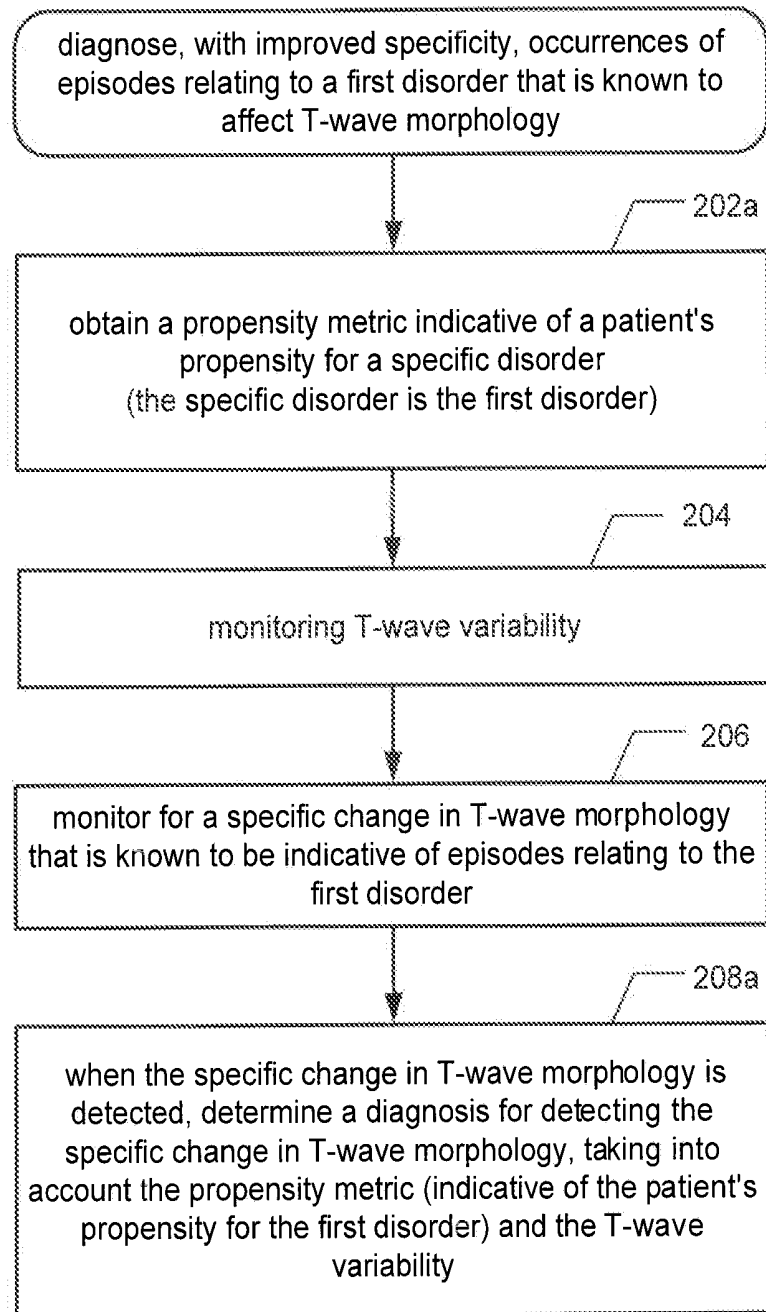


FIG. 1B

**FIG. 2A**

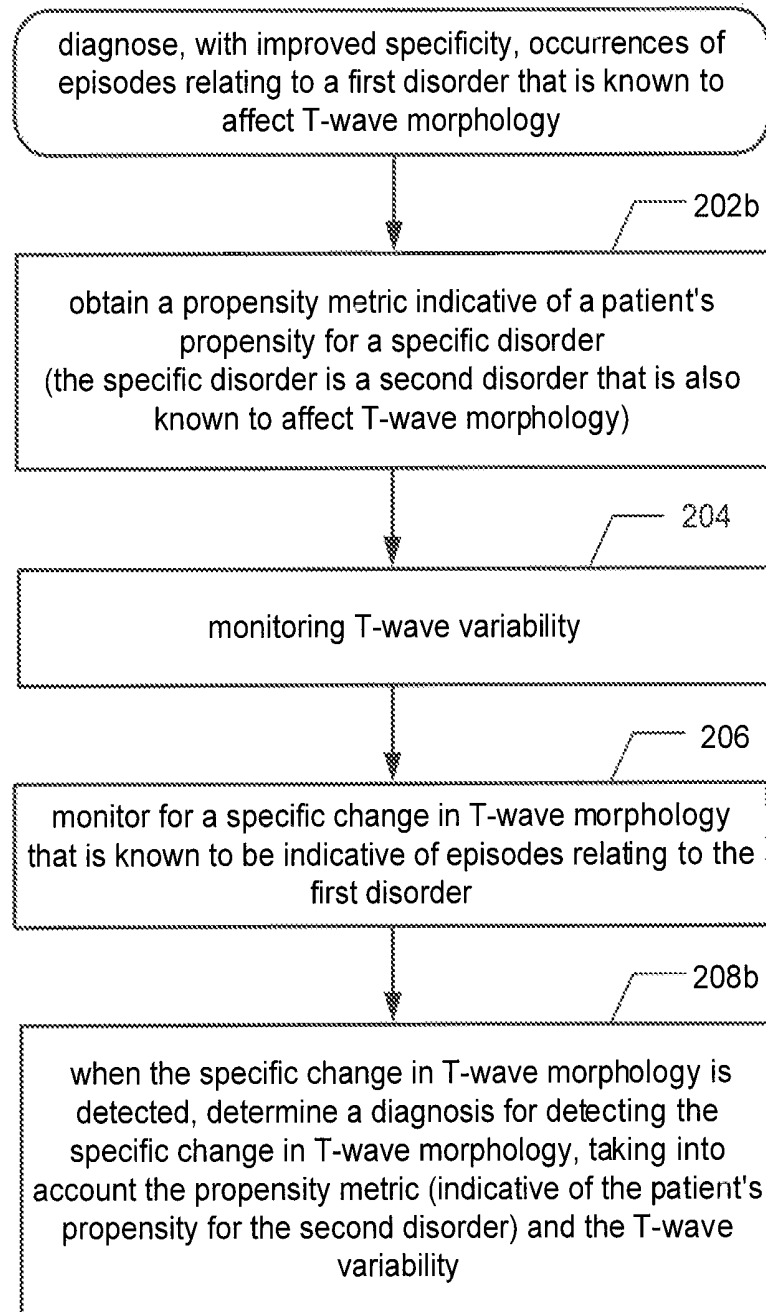


FIG. 2B

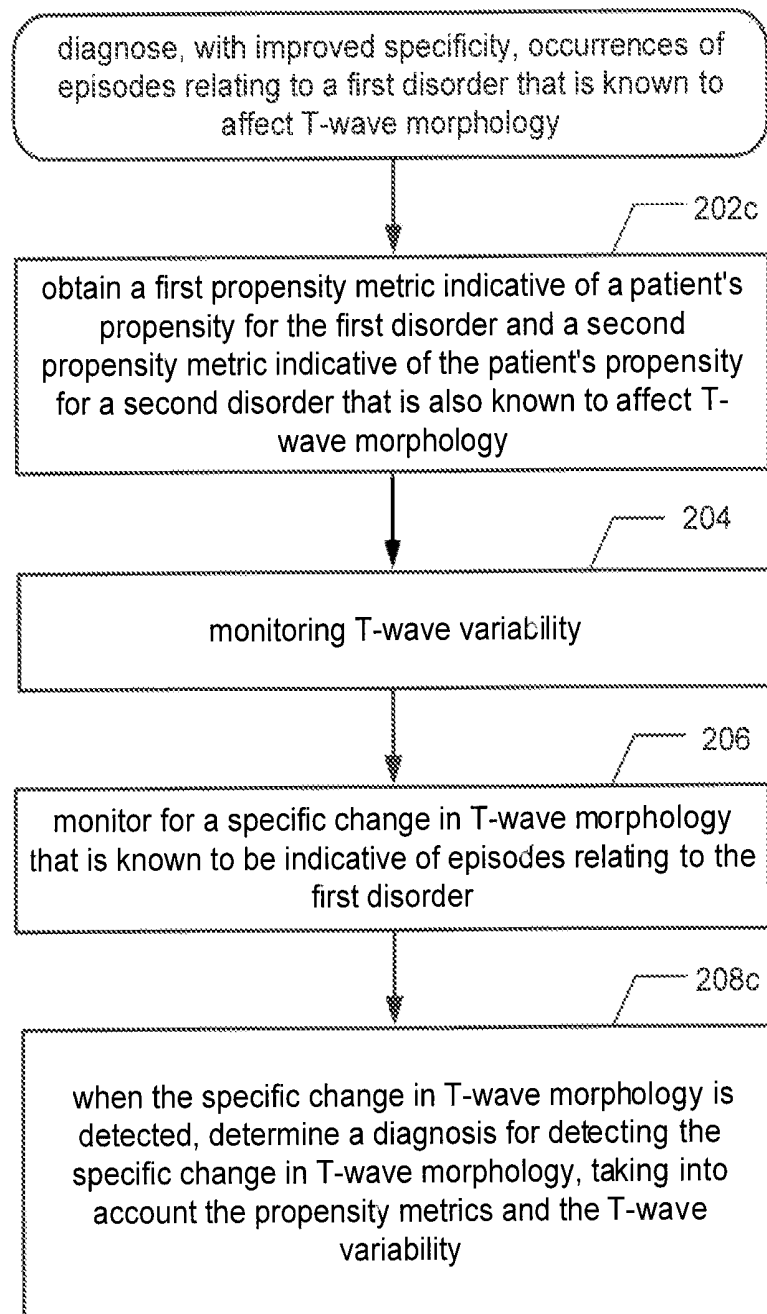
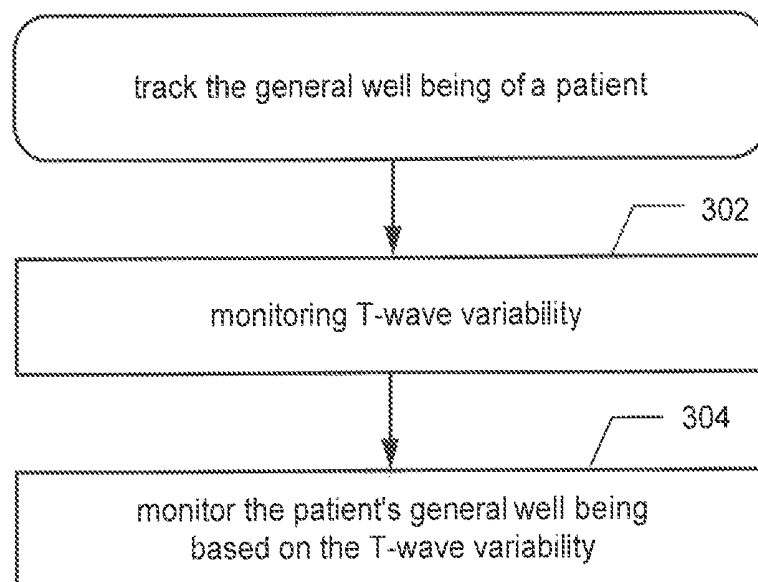


FIG. 2C

**FIG. 3**

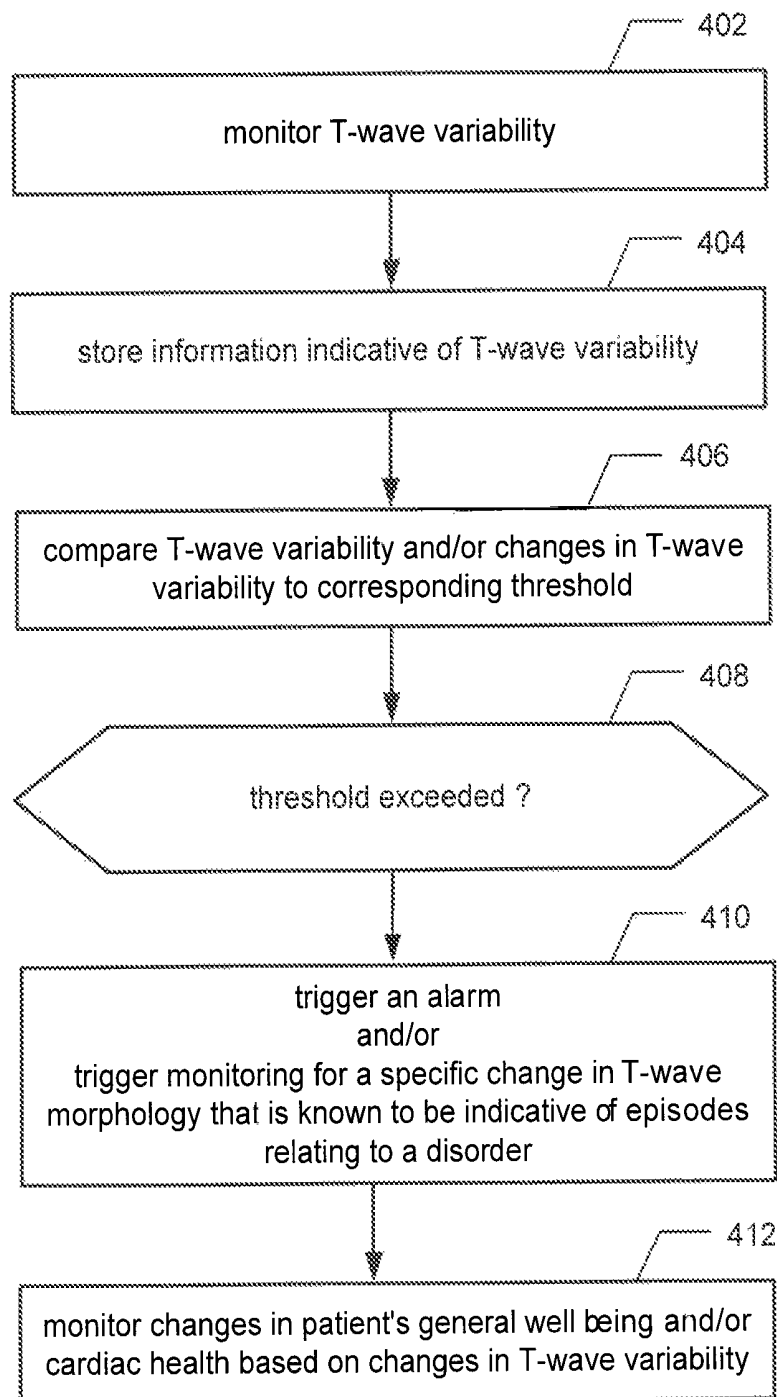


FIG. 4

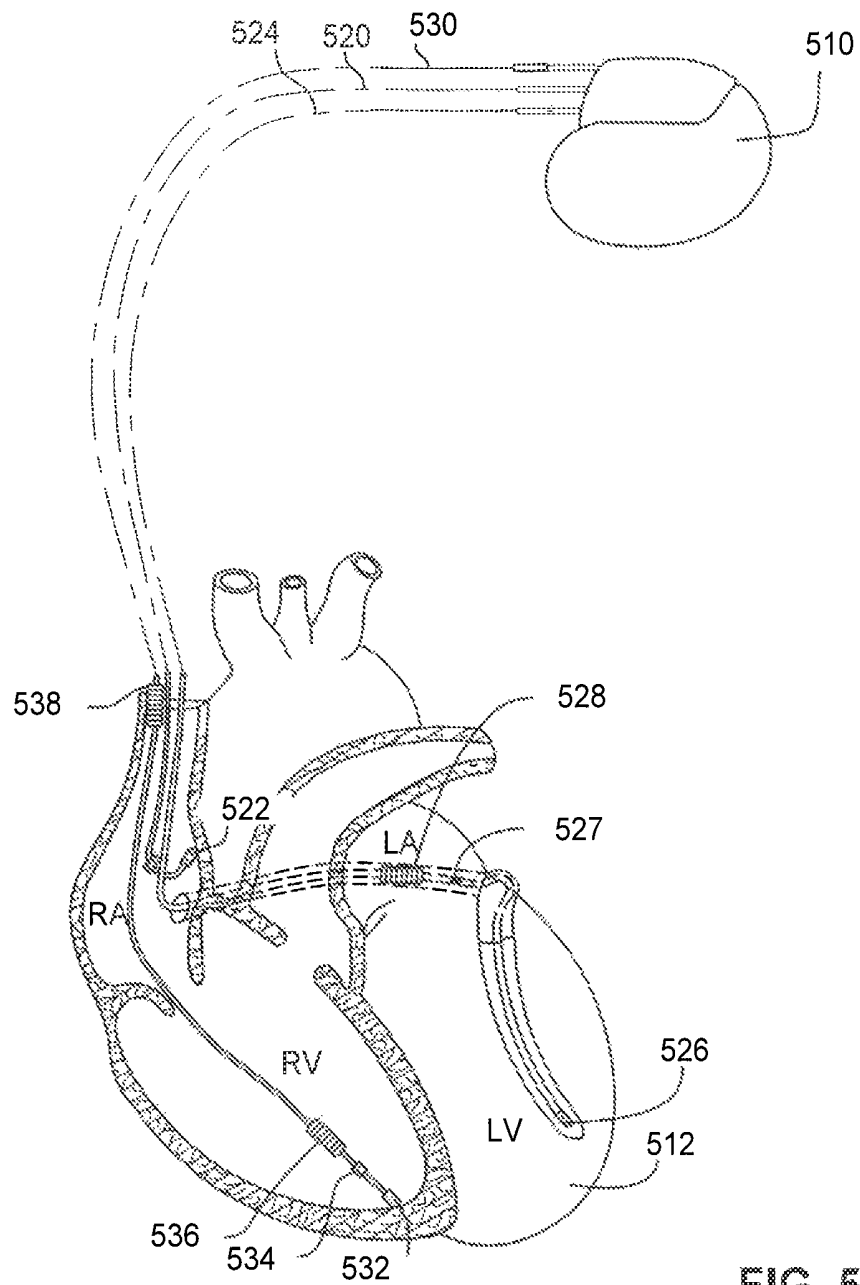


FIG. 5

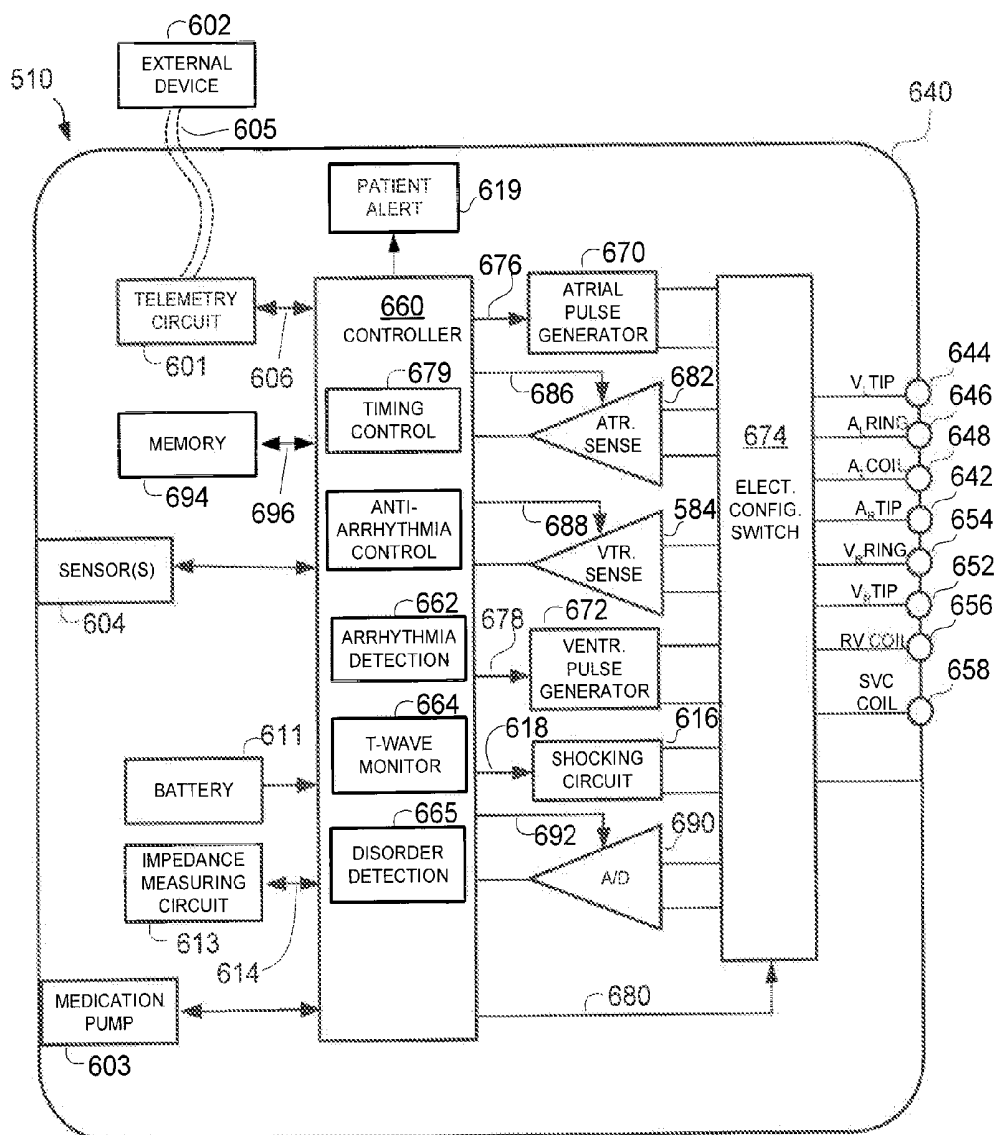


FIG. 6

SYSTEMS AND METHODS FOR INCREASED SPECIFICITY IN DIAGNOSTICS

PRIORITY CLAIM

The present application is a Divisional of, and claims priority to, U.S. patent application Ser. No. 11/928,233, filed Oct. 30, 2007, entitled "SYSTEMS AND METHODS FOR INCREASED SPECIFICITY IN DIAGNOSTICS," now U.S. Pat. No. 8,165,664, which is incorporated herein by reference in its entirety.

FIELD OF THE INVENTION

Embodiments of the present invention relate to systems and methods for diagnosing, with improved specificity, occurrences of episodes relating to disorders that are known to affect T-wave morphology. Exemplary disorders include, but are not limited to, myocardial ischemia, kidney dysfunction and coronary artery disease.

BACKGROUND

Simple parameter extraction of an IEGM can be a very useful tool in a variety of diagnostic features. Many algorithms in implantable or external medical devices are being or have been developed for diagnosing various conditions based on information extracted from the IEGM and various segments within a cardiac cycle. Many of these algorithms, such as ischemia detection, electrolyte imbalance, hypo- and hyper-glycemia, etc., are based on parameters extracted from the repolarization segment (the T-wave) of the IEGM. Because of the sensitivity of the T-wave to changes in O₂, electrolytes, glucose, etc., such algorithms generally have a high sensitivity but lack good specificity. It would be beneficial if the specificity of such algorithms can be increased. More generally, it would be beneficial to increase the specificity of diagnostics based at least in part on measures of T-wave metrics of an IEGM.

SUMMARY

Some embodiments of the present invention relate to systems and methods for diagnosing, with improved specificity, occurrences of episodes relating to disorders that are known to affect T-wave morphology. Other embodiments use similar techniques to monitor patients overtime to facilitate early detection of disease onset, to track the patient's cardiac health and/or to track the patient's general wellbeing.

In accordance with certain embodiments of the present invention, one or more propensity metric(s), each of which is indicative of a patient's propensity for a disorder, is/are obtained, where such disorder(s) is/are known to affect T-wave morphology.

In accordance with certain embodiments of the present invention, a patient's T-wave variability is monitored. This can include measuring one or more T-wave metric of T-waves in one or more IEGM and/or ECG obtained for the patient, and determining the T-wave variability based on the measured T-wave metrics. T-waves are the repolarization segments of a cardiac cycle of an ECG or an IEGM. Such an IEGM can be a ventricular IEGM or an atrial IEGM, or both. Exemplary T-wave metrics, upon which T-wave variability can be based, include peak-to-peak amplitude of T-wave, maximum amplitude of T-wave, location of maximum amplitude of T-wave, minimum amplitude of T-wave, location of minimum amplitude of T-wave, area under T-wave, slope of

T-wave, T-wave centroid, QT interval, corrected QT interval, amplitude of ST segment, QT max-QT end, T-wave frequency content and T-wave frequency spread.

Additionally, a specific change in T-wave morphology is monitored for, where the specific change is known to be indicative of episodes relating to a disorder. In accordance with certain embodiments, when the specific change in T-wave morphology is detected, a diagnosis for detecting the specific change in T-wave morphology is determined, taking into account the propensity metric(s) and the T-wave variability. In accordance with certain embodiments, a level of confidence can be determined for the diagnosis. For example, a diagnosis can have a high, medium or low level of confidence. More or less confidence levels are also possible.

Exemplary disorders, episodes of which can be diagnosed with improved specificity using embodiments of the present invention, include, but are not limited to, diabetes, myocardial ischemia, kidney dysfunction and coronary artery disease. For example, embodiments of the present invention can be used to detect hypoglycemic episodes and hyperglycemic episodes with improved specificity. Embodiments of the present invention can also be used to detect ischemic episodes with improved specificity. Additionally, embodiments of the present invention can be used to detect hyperkalemic episodes and hypokalemic episodes with improved specificity, as well as episodes of angina with improved specificity. Other exemplary disorders that can be detected using embodiment of the present invention include heart failure (HF), myocardial inhomogeneity, and electrolytic imbalances, but are not limited thereto.

In accordance with certain embodiments, measures of T-wave variability can be used to track the general wellbeing and/or the cardiac health of a patient. Additionally, or alternatively, monitored T-wave variability can be used to trigger an alarm, and/or to trigger the monitoring for a specific change in T-wave morphology that is known to be indicative of episodes relating to a disorder. Information indicative of the T-wave variability can be stored, so that changes in the T-wave variability over time can be determined based on the stored information. Increases in T-wave variability can be interpreted as being indicative of a worsening of a patient's cardiac health (and/or general wellbeing), and decreases in T-wave variability can be interpreted as being indicative of an improvement of the patient's cardiac health (and/or general wellbeing).

This description is not intended to be a complete description of, or limit the scope of, the invention. Other features, aspects, and objects of the invention can be obtained from a review of the specification, the figures, and the claims.

BRIEF DESCRIPTION OF THE DRAWINGS

FIG. 1A illustrates an exemplary portion of an ECG signal, including some of its morphologic features. FIG. 1B illustrates exemplary portions of an atrial IEGM and a ventricular IEGM, including some of their morphological features.

FIGS. 2A-2C are high level flow diagrams that are used to explain various embodiments of the present invention.

FIG. 3 is a high level flow diagram is used to explain how measures of T-wave variability can be used to monitor a patient's general wellbeing, in accordance with an embodiment of the present invention.

FIG. 4 is a high level flow diagram that is used to explain how measures of T-wave variability can be used to trigger the monitoring of a disorder, to monitor a patient's cardiac health and/or to monitor a patient's general wellbeing, in accordance with embodiments of the present invention.

FIG. 5 is a simplified, partly cutaway view illustrating an exemplary implantable stimulation device that can be used to implement embodiments of the present invention, where the device is in electrical communication with at least three leads implanted into a patient's heart for delivering multi-chamber stimulation and shock therapy.

FIG. 6 is a functional block diagram of the multi-chamber implantable stimulation device of FIG. 5, illustrating the basic elements that provide pacing stimulation, cardioversion, and defibrillation in four chambers of the heart.

DETAILED DESCRIPTION

The following description is of the best modes presently contemplated for practicing various embodiments of the present invention. The description is not to be taken in a limiting sense but is made merely for the purpose of describing the general principles of the invention. The scope of the invention should be ascertained with reference to the claims. In the description of the invention that follows, like numerals or reference designators will be used to refer to like parts or elements throughout. In addition, the first digit of a reference number identifies the drawing in which the reference number first appears.

It would be apparent to one of skill in the art that the present invention, as described below, may be implemented in many different embodiments of hardware, software, firmware, and/or the entities illustrated in the figures. Any actual software, firmware and/or hardware described herein is not limiting of the present invention. Thus, the operation and behavior of the present invention will be described with the understanding that modifications and variations of the embodiments are possible, given the level of detail presented herein.

A comorbidity is a disorder or disease, in addition to a primary disease or disorder. As used herein, the terms "disorder" and "disease" are used interchangeably. Exemplary disorders include, but are not limited to, diabetes, myocardial ischemia, kidney dysfunction and coronary artery disease. Any one of these exemplary disorders can be a patient's primary disease, with one or more of the other disorders being comorbidities. Other primary disorders and comorbid disorders are also possible, and likely.

Disorders can result in episodes relating to the disorder, also referred to as disorder events. For example, when diabetes is a disorder of a patient, that patient may experience episodes relating to the disorder, such as hypoglycemic episodes. For another example, when a patient has myocardial ischemia, that patient may experience ischemic episodes. In another example, when a patient has kidney dysfunction, that patient may experience hyperkalemic episodes and/or hypokalemic episodes. For a last example, when a patient has coronary artery disease, that patient may experience episodes of angina.

Episodes relating to each of the above mentioned disorders affect the morphology of an intracardiac electrogram (IEGM) and an electrocardiogram (ECG), which are detectable/obtainable signals indicative of the electrical activity of a patient's heart. More specifically, episodes relating to the above mentioned disorders typically affect the repolarization segments of such signals, i.e., the T-wave morphology. Even more specifically, for each of the above disorders, there is a specific change in T-wave morphology that is known to be indicative of episodes relating to the disorder. For example, QT interval prolongation is known to be indicative of a hypoglycemic episode. Additionally, increases in corrected QT interval dispersion are known to be indicative of a hyperglycemic episode. For another example, ST segment deviation is known to be indicative of an ischemic episode. Additionally, ST segment elevation is known to be indicative of a hyperkalemic episode, and ST segment depression is known to be indicative of a hypokalemic episode. ST segment depression is also known to be indicative of episodes of angina.

Because it is known how various disorders can affect T-wave morphology, many detection algorithms rely on measures of T-wave morphology to detect episodes of a disorder (where the disorder can be the primary disorder or a comorbidity). For example, an ischemic episode detection algorithm can monitor for ST segment deviations. Such algorithms may have a relatively high sensitivity. However, since T-wave morphology can be affected by many other factors, such as O₂, electrolytes, glucose, etc., as well as episodes of other disorders (e.g., comorbidities), these detection algorithms often have lower than desired specificities.

As used herein, sensitivity refers to the likelihood that an episode relating to a disorder (e.g., an ischemic episode) will actually be characterized as the episode relating to the disorder; and specificity refers to the likelihood that only the episodes relating to the disorder (as opposed to episodes relating to another disorder) will actually be characterized as episodes relating to the disorder. For example, an ischemia detection algorithm can have a 100% sensitivity and an 80% specificity if it always characterizes ischemic episodes as ischemic episodes, but also characterizes some hyperkalemic episodes as ischemic episodes. For another example, an ischemic detection algorithm can have an 80% sensitivity and a 100% specificity if it never mischaracterizes hyperkalemic or other episodes as ischemic episodes, but misses detecting some episodes of ischemia.

Specific embodiments of the present invention relate to systems and methods for diagnosing, with improved specificity, occurrences of episodes relating to a disorder that is known to affect T-wave morphology. Such embodiments keep track of the variability of one or more T-wave metric over time. Additionally, such embodiments take into account the patient's propensity for the specific disorder and/or the patient's propensity for another disorder that is also known to affect T-wave morphology.

FIG. 1A illustrates an exemplary portion of an ECG signal, including some of its morphologic features. FIG. 1B illustrates exemplary portions of an atrial IEGM and a ventricular IEGM, including some of their morphological features. Included in the illustrations is a P-wave, a Q-, R- and S-wave (which make up a QRS complex) and a T-wave. Also shown are some of the various metrics of the signal that can be measured, including PR interval, PR segment, ST segment, QT interval, maximum amplitude of T-wave (Tmax), minimum amplitude of T-wave (Tmin), and peak-to-peak amplitude of T-wave (T peak-to-peak). As can be appreciated, many of these metrics relate to the T-wave morphology. Thus, many of these metrics may be affected by disorders that are known to affect T-wave morphology. Additional metrics of T-wave morphology include, but are not limited to, location of maximum amplitude of T-wave, location of minimum amplitude of T-wave, area under T-wave, slope of T-wave, T-wave amplitude dispersion, T-wave centroid, QT interval, QT interval dispersion, corrected QT interval dispersion, amplitude of ST segment, T-wave frequency content, and T-wave frequency spread. As will be appreciated from the following discussion, one or more of these metrics may be affected by specific disorders, and thus, can be used to attempt to detect episodes relating to specific disorders.

The high level flow diagrams of FIGS. 2A and 2B will now be used to summarize various embodiments of the present

invention that relate to diagnosing, with improved specificity, occurrences of episodes relating to a “first disorder” that is known to affect T-wave morphology. Such a first disorder can be a primary disorder, or a comorbidity. Although not necessary, it will be assumed, for the discussion of the flow diagrams of FIGS. 2A and 2B, that patient has a propensity for the first disorder as well as a propensity for another (i.e., second) disorder. One of these disorders can be the primary disorder, and the other can be a comorbidity, or both the first and second disorders can be comorbidities.

The flow diagrams of FIGS. 2A-2C provide an overview of the operation and novel features that can be implemented in various embodiments, e.g., of an implantable device and/or external device. In the flow diagrams, the various algorithmic steps are summarized in individual ‘blocks’. Such blocks describe specific actions or decisions that are made or carried out as the algorithm proceeds. Where a microcontroller (or equivalent) is employed, the flow diagram presented herein provides the basis for a ‘control program’ that may be used by such a microcontroller (or equivalent) to effectuate the desired control of the stimulation device. Those skilled in the art may readily write such a control program based on the flow diagram and other descriptions presented herein.

Where steps of the flow diagrams 2A-2C are the same, they are numbered the same. Where steps of these flow diagrams differ, the steps are labeled with either an “a”, “b” or “c” following the base reference number.

Referring first to FIG. 2A, at step 202a, a propensity metric indicative of a patient’s propensity for a specific disorder is obtained. The specific disorder can be the first disorder (for which there is an attempt to improve the specificity of diagnosing occurrences of episodes relating to the disorder). Alternatively, the specific disorder, for which a propensity metric is obtained, can be a second disorder that is also known to affect T-wave morphology, as indicated at step 202b in FIG. 2B.

For example, assume that there is a desire to improve the specificity of diagnosing occurrences of episodes relating to diabetes. Such episodes can be hyperglycemic episodes or hypoglycemic episodes, both of which can occur in diabetic patients. The propensity metric, obtained at step 202a, can be indicative of a patient’s propensity for diabetes. Alternatively, the propensity metric, obtained at step 202b, can be indicative of the patient’s propensity for another disorder, such as coronary artery disease, that is also known to affect T-wave morphology.

In certain embodiments the propensity metric can have one of four possible values, however use of more or less values is also within the scope of the present invention. The scale of the propensity metric can be selected as desired. For example, in one embodiment, the lowest propensity metric is 0 and the highest propensity metric is 1, i.e., the scale is 0-1. In another embodiment, the lowest propensity metric is 0 and the highest propensity metric is 3, i.e., the scale is 0-3. An example of a 0-3 scale is shown below in Table 1. Other scales are possible, and within the scope of the present invention.

TABLE 1

Propensity Metric Value	Corresponding Condition
0	The patient has not been diagnosed with the disorder, and does not have a predisposition for developing the disorder later
1	The patient has not been diagnosed with the disorder, but the patient has a predisposition for developing the disorder later
2	The patient has not been diagnosed with the

TABLE 1-continued

Propensity Metric Value	Corresponding Condition
3	disorder, but the patient has a high risk of developing the disease later The patient currently has been diagnosed with the disorder

A physician can determine the propensity metric for a specific disorder, e.g., based on a patient’s own history, the patient’s family history, a questionnaire and/or tests performed on the patient. The propensity metric can be determined at the time of implant of an implantable cardiac device, and can be updated at follow-up visits.

Referring again to FIGS. 2A and 2B, as shown at step 204, a patient’s T-wave variability is monitored. This can include determining a T-wave variability index (TVi), which can be determined on a continuous, periodic or aperiodic basis. The TVi, or more generally the T-wave variability, can be a measure of variability of one or more T-wave metric. Exemplary T-wave metrics, of which a variability can be calculated, include, but are not limited to: maximum amplitude of T-wave, minimum amplitude of T-wave, peak-to-peak amplitude of T-wave, location of maximum amplitude of T-wave, location of minimum amplitude of T-wave, area under T-wave, slope of T-wave, T-wave amplitude dispersion, T-wave centroid, QT interval, corrected QT interval, amplitude of ST segment, T-wave frequency content, and T-wave frequency spread. Another exemplary T-wave metric (whose variability can be determined and monitored) is QT max–QT end. There are various techniques that are known for identifying T-waves, thereby enabling measurement of the above mentioned T-wave metrics. Some exemplary techniques for detecting T-waves are disclosed in U.S. patent application Ser. No. 10/979,833, entitled “Systems and Methods for Automatically Setting Refractory and Blanking Periods,” (Snell and Bharmi) filed Nov. 1, 2004, now abandoned, which is incorporated herein by reference. Some additional exemplary techniques for detecting T-waves are disclosed in U.S. Pat. No. 5,782,887 (van Krieken et al) and U.S. Pat. No. 6,836,682 (Van Dam), which are incorporated herein by reference. Use of alternative techniques for detecting T waves are also within the scope of the present invention.

For each of the above T-wave metrics, actual, absolute, normalized (e.g., to heart rate and/or R-wave amplitude), or otherwise adjusted values can be used. The monitored T-wave variability can be, e.g., a variability of any one of the above T-wave metrics, or a weighted average of the variability of multiple ones of the above T-wave metrics. In addition, or instead of using the above T-wave metrics, T-wave variability can be of isochoric points of the T-wave. T-wave variability may also be or include a measure of the variability of a magnitude of T-wave alternans. In other words, magnitudes of T-wave alternans can be a T-wave metric for which a measure of variability is determined.

T-wave variability can be determined by calculating a standard deviation, a pseudo random deviation, root mean-square differences, a range, a interquartile range, a mean difference, a median absolute deviation, an average absolute deviation, etc, of any of the above mentioned T-wave metrics, or combinations thereof, or other T-wave metrics. These are just a few examples, which are not meant to be limiting. Also, it is noted that most any known technique for determining heart rate variability (HRV); including but not limited to time domain, frequency domain, and non-linear techniques, can be

used to determine T-wave variability by using measures of T-wave metrics in place of measures of RR intervals.

In specific embodiments, a T-wave variability can be determined at implant, or at some other time when the patient is known to not be experiencing any episodes of a disorder. This can be considered the patient's baseline T-wave variability.

When T-wave variability is monitored at step 204, this can include determining a value of T-wave variability, comparing the value of T-wave variability to one or more threshold, and/or comparing a difference between the value of T-wave variability and the baseline T-wave variability to a corresponding threshold. The baseline T-wave variability may also be updated from time to time, but preferably should be determined based on T-wave metrics obtained when the patient is not experiencing episodes of a disorder.

As mentioned to above, T-wave variability can be determined substantially continuous and/or periodically. For example, there can be a running value of T-wave variability. Additionally, or alternatively, T-wave variability can be determined every 5 minutes, hourly, daily, weekly and/or monthly, etc. T-wave variability can be determined for a single window of time (e.g., 5 minute window or hour window, etc), or for multiple windows of time (e.g., 5 minute and 1 hour windows, etc).

Through experimentation, a specific disorder's affect on T-wave variability can be determined. For example, the inventors have determined that a baseline T-wave variability for diabetics is higher than normal, and that QT-interval increases further during episodes of hypoglycemia. For other disorders, it may be determined that T-wave variability does not increase, or at least not significantly, during episodes of the disorder. It may even be determined that T-wave variability stays the same or decreases during episodes of a certain disorder. From this, it can be appreciated that by monitoring T-wave variability, the specificity of a diagnosis can be improved, if T-wave variability is taken into account when determining the diagnosis.

Still referring to FIGS. 2A and 2B, at step 206, monitoring for a specific change in T-wave morphology is performed, where the specific change in T-wave morphology is known to be indicative of episodes relating to the first disorder. For example, it is known that QT interval prolongation is indicative of hypoglycemic episodes, and that an increase in corrected QT interval dispersion is indicative of hyperglycemic episodes. Thus, at step 206, if the patient has diabetes (i.e., assume the first disorder referred to in FIGS. 2A-2C is diabetes), then an elongation of the QT interval and/or an increase in correct QT interval dispersion can be monitored for at step 206. Additional examples are discussed below.

As specified at steps 208a and 208b, when the specific change in T-wave morphology is detected (e.g., ST segment depression), a diagnosis for detecting the specific change in T-wave morphology is determined, taking into account the propensity metric and the T-wave variability. Steps 208a and 208b differ in that in step 208a, the propensity metric relates to the first disorder, and in step 208b the propensity metric relates to the second disorder that is also known to affect T-wave morphology. The differences between these will be explained by way of a few examples.

For example, assume that a patient is likely to develop a kidney dysfunction disorder, and that the desire is to detect hypokalemic episodes with increased specificity. It is known that during a hypokalemic episode a patient typically exhibits ST segment depression. Note that it is also known that during an episode of angina, which occur in patients having coronary artery disease, a patient also typically exhibits ST segment depression. In one embodiment, the propensity metric

obtained at step 202a can be indicative of the patient's propensity for kidney dysfunction. Where that is the case, if ST segment depression is detected, then at step 208a, the patient's propensity for kidney dysfunction, and the monitored T-wave variability, are taken into account when determining the diagnosis for the detected ST segment depression. Also, assume that it has been determined how hypokalemic episodes affect T-wave variability (e.g., hypokalemic episodes increase T-wave variability). If the patient has a high propensity for kidney dysfunction, the patient's T-wave variability is high (or relatively high compared to the baseline), then a diagnosis that the patient experienced a hypokalemic episode can be made with high confidence.

In another example, assume again that a patient is likely to develop a kidney dysfunction disorder, and that the desire is to detect hypokalemic episodes with increased specificity. Again, assume that it has been determined how hypokalemic episodes affect T-wave variability (e.g., assume hypokalemic episodes increase T-wave variability). However, here assume that the propensity metric obtained at step 202b is indicative of the patient's propensity for coronary artery disease, which as mentioned above, reveals itself as episodes of angina. As also mentioned above, episodes of angina typically cause ST segment depression. If the patient has a high propensity for coronary artery disease, and the T-wave variability is high (or relatively high compared to the baseline), then at step 208b a diagnosis that the patient experienced a hypokalemic episode (when ST segment depression is detected) may be made with low confidence, since there is a fairly good likelihood that an episode of angina may have caused the ST segment depression. However, if the patient has no propensity, or a very low propensity for angina, then at step 208b a diagnosis that the patient experienced a hypokalemic episode (when ST segment depression is detected) can be made with high confidence, since it is unlikely that it was an episode of angina that caused the ST segment depression. In this last example, if the patient's T-wave variability were relatively low (or more generally, the T-wave variability is not what is expected for an episode of a hypokalemic episode), then the confidence level of the diagnosis can be affected.

It also possible to obtain multiple propensity metrics, and that the multiple propensity metrics can be taken into account, along with T-wave variability, when producing a diagnosis for detecting a specific change in T-wave morphology. Continuing with the above example, if the patient has a high propensity for kidney dysfunction, and a low propensity for coronary artery disease, then a detection of ST segment depression and high T-wave variability can be diagnosed as a hypokalemic episode with high confidence. However, if the patient has a medium propensity for kidney dysfunction, and a medium propensity for coronary artery disease, then a detected ST segment depression can be diagnosed as a hypokalemic episode with medium confidence. A summary of such embodiments is provided in FIG.

An exemplary algorithm for determining a diagnosis is:

$$\text{diagnosis score for disorder}_i = (\text{propensity} * \text{weight1}) + (\text{TV}_i * \text{weight2}) + (\text{presence of expected change in T-wave morphology} * \text{weight3}).$$

There can be a similar algorithm for each disorder that is being monitored for. The "diagnosis score" can be compared to one or more threshold, to determine whether a specific diagnosis should be made, and/or to determine a confidence level of a diagnosis. Multiple propensities, each having a different weight, can be used in such an algorithm. Where the presence of something (e.g., a certain T-wave morphology, or a high N_i) makes a diagnosis less likely, negative weighting

factors can be used. The above algorithm is just one example of an algorithm that can be used at steps **208a**, **208b** and **208c**. One of ordinary skill in the art reading this disclosure will understand that numerous alternative algorithms can be used that take into account one or more propensity metric and T-wave variability, when producing a diagnosis. Use of such alternative algorithms is within the scope of the present invention.

As mentioned above, embodiments of the present invention can be used to diagnose, with improved specificity, occurrences of episodes relating to disorders that are known to affect T-wave morphology. Exemplary disorders include, but are not limited to, diabetes, myocardial ischemia, kidney dysfunction, coronary artery disease, diastolic heart failure, systolic heart failure, myocardial inhomogeneity and various electrolytic imbalances. Exemplary details of how embodiments of the present invention can be used to detect hypokalemic episodes, in patients that have or are likely to develop a kidney dysfunction disorder, were provided above. Additional details of how the present invention can be used to diagnose occurrences of episodes of some of the other exemplary disorders are provided below, again with reference to FIGS. 2A-2C.

Where a patient has diabetes, or may develop diabetes, embodiments of the present invention can be used to diagnose, with improved specificity, hypoglycemic episodes. Referring to FIG. 2A, the propensity metric obtained at step **202a** can be indicative of the patient's propensity for diabetes. Alternatively (as indicated at step **202b** in FIG. 2B), or additionally (as indicated at step **202c** in FIG. 3C), an obtained propensity metric can be indicative of the patient's propensity for a second disorder that is also known to affect T-wave morphology. It is known that during hypoglycemic episodes, a patient typically experiences QT interval prolongation. Also, assume that it has been determined that hypoglycemic episodes increase T-wave variability. Accordingly, at step **206** (in FIGS. 2A-2C), the specific change in T-wave morphology that is monitored for can be QT interval prolongation. At step **208a** (in FIG. 2A), when a prolongation of the QT interval (e.g., beyond a threshold) is detected, a diagnosis for detecting QT interval prolongation can be made, taking into account the patient's propensity for diabetes and the correspond T-wave variability (determined at step **206**). Alternatively, at step **208b** (in FIG. 2B), when QT interval prolongation is detected, a diagnosis for such a detection can be made, taking into account the patient's propensity for another disorder (besides diabetes) and the correspond T-wave variability (determined at step **206**). In still another embodiment, at step **208c** (in FIG. 2C), when QT interval prolongation is detected, a diagnosis for detecting QT interval prolongation can be made, taking into account the patient's propensity for diabetes and the patient's propensity for another disorder (besides diabetes), and the correspond T-wave variability.

When the patient has diabetes, or may develop diabetes, embodiments of the present invention can also be used to diagnose, with improved specificity, hyperglycemic episodes, which are known to typically cause an increase in corrected QT (QTc) interval dispersion. Accordingly, at step **206** (in FIGS. 2A-2C), the specific change in T-wave morphology that is monitored for can be an increase in QTc interval dispersion. Also, assume that it has been determined that hyperglycemic episodes increase T-wave variability. At step **208a** (in FIG. 2A), when an increase in QTc interval dispersion (e.g., beyond a threshold) is detected, a diagnosis for detecting the increase in QTc interval dispersion can be made, taking into account the patient's propensity for diabetes and the correspond T-wave variability (determined at step

206). Alternatively, at step **208b** (in FIG. 2B), the diagnosis for such a detection can be made, taking into account the patient's propensity for another disorder (besides diabetes) and the correspond T-wave variability (determined at step **206**). In still another embodiment, at step **208c** (in FIG. 2C), when the increase in QTc interval dispersion is detected, a diagnosis can be made, taking into account the patient's propensity for diabetes and the patient's propensity for another disorder (besides diabetes), and the correspond T-wave variability.

Where a patient has or may develop myocardial ischemia, embodiments of the present invention can be used to diagnose, with improved specificity, ischemic episodes. Referring to FIG. 2A, the propensity metric obtained at step **202a** can be indicative of the patient's propensity for myocardial ischemia. Alternatively (as indicated at step **202b** in FIG. 2B), or additionally (as indicated at step **202c** in FIG. 3C), an obtained propensity metric can be indicative of the patient's propensity for a second disorder that is also known to affect T-wave morphology. It is known that during ischemic episodes, a patient typically experiences ST segment deviation. Accordingly, at step **206** (in FIGS. 2A-2C), the specific change in T-wave morphology that is monitored for can be ST segment deviation. Also, assume that it has been determined how hypoglycemic episodes affect T-wave variability. At step **208a** (in FIG. 2A), when a deviation of the ST interval (e.g., beyond a threshold) is detected, a diagnosis for detecting ST segment deviation can be made, taking into account the patient's propensity for myocardial ischemia and the correspond T-wave variability (determined at step **206**). Alternatively, at step **208b** (in FIG. 2B), when ST segment deviation is detected, a diagnosis for such a detection can be made, taking into account the patient's propensity for another disorder (besides myocardial ischemia) and the correspond T-wave variability (determined at step **206**). In still another embodiment, at step **208c** (in FIG. 2C), when ST segment deviation is detected, a diagnosis for such a detection can be made, taking into account the patient's propensity for myocardial ischemia and the patient's propensity for another disorder (besides myocardial ischemia), and the correspond T-wave variability.

Provided above was a discussion of how to increase the specificity of diagnosing episodes of hypokalemic episodes for patient's that have or are likely to develop a kidney dysfunction disorder. Such patient's may also experience hyperkalemic episodes, which are known to typically cause ST segment elevation. Accordingly, embodiments of the present invention can be used to diagnose, with improved specificity, hyperkalemic episodes. Referring to FIG. 2A, the propensity metric obtained at step **202a** can be indicative of the patient's propensity for kidney dysfunction. Alternatively (as indicated at step **202b** in FIG. 2B), or additionally (as indicated at step **202c** in FIG. 3C), an obtained propensity metric can be indicative of the patient's propensity for a second disorder that is also known to affect T-wave morphology. As mentioned above, it is known that during hyperkalemic episodes, a patient typically experiences ST segment elevation. Accordingly, at step **206** (in FIGS. 2A-2C), the specific change in T-wave morphology that is monitored for can be ST segment elevation. Also, assume that it has been determined how hyperkalemic episodes affect T-wave variability. At step **208a** (in FIG. 2A), when an elevation of the ST interval (e.g., beyond a threshold) is detected, a diagnosis for detecting ST segment elevation can be made, taking into account the patient's propensity for kidney dysfunction and the corresponding T-wave variability (determined at step **206**). Alternatively, at step **208b** (in FIG. 2B), when ST segment eleva-

tion is detected, a diagnosis for such a detection can be made, taking into account the patient's propensity for another disorder (besides kidney dysfunction) and the corresponding T-wave variability (determined at step 206). In still another embodiment, at step 208c (in FIG. 2C), when ST segment elevation is detected, a diagnosis for such a detection can be made, taking into account the patient's propensity for kidney dysfunction and the patient's propensity for another disorder (besides kidney dysfunction), and the correspond T-wave variability.

Where a patient has or may develop coronary artery disease, embodiments of the present invention can be used to diagnose, with improved specificity, episodes of angina. Referring to FIG. 2A, the propensity metric obtained at step 202a can be indicative of the patient's propensity for coronary artery disease. Alternatively (as indicated at step 202b in FIG. 2B), or additionally (as indicated at step 202c in FIG. 3C), an obtained propensity metric can be indicative of the patient's propensity for a second disorder that is also known to affect T-wave morphology. It is known that during episodes of angina, a patient typically experiences ST segment depression. Accordingly, at step 206 (in FIGS. 2A-2C), the specific change in T-wave morphology that is monitored for can be ST segment depression. Also, assume that it has been determined how episodes of angina affect T-wave variability. At step 208a (in FIG. 2A), when a depression of the ST segment (e.g., beyond a threshold) is detected, a diagnosis for detecting ST segment depression can be made, taking into account the patient's propensity for coronary artery disease and the corresponding T-wave variability (determined at step 206). Alternatively, at step 208b (in FIG. 2B), when ST segment depression is detected, a diagnosis for such a detection can be made, taking into account the patient's propensity for another disorder (besides coronary artery disease) and the corresponding T-wave variability (determined at step 206). In still another embodiment, at step 208c (in FIG. 2C), when ST segment depression is detected, a diagnosis for detecting ST segment depression can be made, taking into account the patient's propensity for coronary artery disease and the patient's propensity for another disorder (besides coronary artery disease), and the corresponding T-wave variability.

Based on the above discussion, one of ordinary skill in the art will appreciate how embodiments of the present invention can be used to increase the specificity of diagnosing episodes of disorders, other than those discussed in detail above. For example, embodiments of the present invention can also be used to diagnose episodes of diastolic heart failure, systolic heart failure, myocardial inhomogeneity, and various electrolytic imbalances, with increased specificity. Also, in the above discussion, exemplary indicators of each disorder were discussed (e.g., ST segment depression is indicative of episodes of angina). However, monitoring for other indicators and/or additional indicators, other than those mentioned above, are also within the scope of the present invention.

Embodiments of the present invention can be used to monitor for a plurality of different specific changes in T-wave morphology at the same time, where each monitored for change in T-wave morphology is known to be indicative an episode relating to a disorder (e.g., a first change may correspond to an episode of a first disorder, a second change may correspond to an episode of a second disorder, etc.). In other words, multiple instances of embodiments of the present invention can occur in parallel. Then, whenever a change in T-wave morphology is detected, a diagnosis can be made for the detection, taking into account one or more propensity metric and the patient's T-wave variability.

More generally, embodiments of the present invention described above can be used to produce a diagnosis, taking into account T-wave morphology, T-wave variability and one or more propensity metric. Such embodiments should provide for improved specificity of a diagnosis.

When an episodes of a disorder is detected, information about the episode, including but not limited to the time of the episode, the length of the episode, information about the detected change in T-wave morphology, T-wave variability (e.g., TVi) and the like, can be stored for later retrieval and/or analysis, e.g., by a physician. Additionally, depending on what episode is detected, an alarm and/or therapy can be triggered. The above described embodiments of the present invention do not relate to the specific alarms and/or therapy that are triggered. Rather, the above described embodiments of the present invention relate to increasing the specificity of diagnosing the occurrences of such episodes, e.g., so that more specific and appropriate therapy can be delivered.

As described with reference to the high level flow diagram of FIG. 3, a metric of T-wave variability (e.g., TM) can also be used to track the general wellbeing of the patient. This can include monitoring T-wave variability at step 302, which can include monitoring the time course of its change away and back to baseline. Then, based on the T-wave variability, the general wellbeing of the patient can be monitored, as indicated at step 304. Information about T-wave variability can thus be saved and trended. It is expected a patient's T-wave variability will decrease, if a patient's general wellbeing improves, and vice versa. Accordingly, an increase in Ni can be interpreted as being indicative of a worsening of a patient's general wellbeing, and a decrease in TVi can be interpreted as being indicative of improvement of a patient's general wellbeing.

In certain embodiments, measures of T-wave variability can be used as a trigger to monitor for episodes relating to a disorder that is known to affect T-wave morphology. In other words, when T-wave variability exceeds a specified threshold, this can trigger attempting to determine the cause of the increase in T-wave variability. This can also trigger an alarm. More specifically, referring to FIG. 4, measures of T-wave variability can be used to trigger an alarm and/or the monitoring for a specific change in T-wave morphology that is known to be indicative of episodes relating to a disorder, as indicated at steps 406-410 of FIG. 4. More generally, when T-wave variability, or a change therein, exceeds a corresponding threshold, a diagnosis can be produced. For example, as was described above, the diagnosis can be produced taking into account T-wave morphology, T-wave variability and propensity metrics. Additionally, information that is indicative of the T-wave variability can be stored, as indicated at step 404, and changes in the T-wave variability over time can be monitored based on the stored information, as indicated at steps 412. Also, at step 412, a patient's cardiac health and/or general wellbeing can be monitored based on the changes in T-wave variability. This can include interpreting increases in T-wave variability as being indicative of a worsening of a patient's cardiac health (and/or general wellbeing), and interpreting decreases in T-wave variability as being indicative of an improvement of the patient's cardiac health (and/or general wellbeing).

Exemplary Implantable System

FIGS. 5 and 6 will now be used to describe an exemplary implantable system that can be used to implement the embodiments of the present invention which were described above. Referring to FIG. 5, the implantable system is shown as including an implantable stimulation device 510, which can be a pacing device and/or an implantable cardioverter

defibrillator. The device **510** is shown as being in electrical communication with a patient's heart **512** by way of three leads, **520**, **524** and **530**, which can be suitable for delivering multi-chamber stimulation and shock therapy.

Still referring to FIG. **5**, to sense atrial cardiac signals and to provide right atrial chamber stimulation therapy, the device **510** is coupled to an implantable right atrial lead **520** having at least an atrial tip electrode **522**, which typically is implanted in the patient's right atrial appendage. To sense left atrial and ventricular cardiac signals and to provide left-chamber pacing therapy, the device **510** is coupled to a "coronary sinus" lead **524** designed for placement in the "coronary sinus region" via the coronary sinus for positioning a distal electrode adjacent to the left ventricle and/or additional electrode(s) adjacent to the left atrium. As used herein, the phrase "coronary sinus region" refers to the vasculature of the left ventricle, including any portion of the coronary sinus, great cardiac vein, left marginal vein, left posterior ventricular vein, middle cardiac vein, and/or small cardiac vein or any other cardiac vein accessible by the coronary sinus.

Accordingly, an exemplary coronary sinus lead **524** is designed to receive atrial and ventricular cardiac signals and to deliver left ventricular pacing therapy using at least a left ventricular tip electrode **526**, left atrial pacing therapy using at least a left atrial ring electrode **527**, and shocking therapy using at least a left atrial coil electrode **528**.

The device **510** is also shown in electrical communication with the patient's heart **512** by way of an implantable right ventricular lead **530** having, in this embodiment, a right ventricular tip electrode **532**, a right ventricular ring electrode **534**, a right ventricular (RV) coil electrode **536**, and an SVC coil electrode **538**. Typically, the right ventricular lead **530** is transvenously inserted into the heart **512** so as to place the right ventricular tip electrode **532** in the right ventricular apex so that the RV coil electrode **536** will be positioned in the right ventricle and the SVC coil electrode **538** will be positioned in the superior vena cava. Accordingly, the right ventricular lead **530** is capable of receiving cardiac signals and delivering stimulation in the form of pacing and shock therapy to the right ventricle.

FIG. **6** will now be used to provides some exemplary details of the components of the implantable devices **510**. Referring now to FIG. **6**, each of the above implantable devices **510**, and alternative versions thereof, can include a microcontroller **660**. As is well known in the art, the microcontroller **660** typically includes a microprocessor, or equivalent control circuitry, and can further include RAM or ROM memory, logic and timing circuitry, state machine circuitry, and I/O circuitry. Typically, the microcontroller **660** includes the ability to process or monitor input signals (data) as controlled by a program code stored in a designated block of memory. The details of the design of the microcontroller **660** are not critical to the present invention. Rather, any suitable microcontroller **660** can be used to carry out the functions described herein. The use of microprocessor-based control circuits for performing timing and data analysis functions are well known in the art. In specific embodiments of the present invention, the microcontroller **660** performs some or all of the steps associated monitoring T-wave variability, and with diagnosing, with improved specificity, occurrences of episodes relating to disorders that are known to affect T-wave morphology. Additionally, the microcontroller can be used to monitor changes in the cardiac health of a patient based changes in T-wave variability.

Representative types of control circuitry that may be used with the invention include the microprocessor-based control system of U.S. Pat. No. 4,940,052 (Mann et. al.) and the

state-machines of U.S. Pat. No. 4,712,555 (Sholder) and U.S. Pat. No. 4,944,298 (Sholder). For a more detailed description of the various timing intervals used within the pacing device and their inter-relationship, see U.S. Pat. No. 4,788,980 (Mann et. al.). The '052, '555, '298 and '980 patents are incorporated herein by reference.

Depending on implementation, the device **510** can be capable of treating both fast and slow arrhythmias with stimulation therapy, including pacing, cardioversion and defibrillation stimulation. While a particular multi-chamber device is shown, this is for illustration purposes only, and one of skill in the art could readily duplicate, eliminate or disable the appropriate circuitry in any desired combination to provide a device capable of treating the appropriate chamber(s) with pacing, cardioversion and defibrillation stimulation. For example, where the implantable device is a monitor that does not provide any therapy, it is clear that many of the blocks shown may be eliminated.

The housing **640**, shown schematically in FIG. **6**, is often referred to as the "can", "case" or "case electrode" and may be programmably selected to act as the return electrode for all "unipolar" modes. The housing **640** may further be used as a return electrode alone or in combination with one or more of the coil electrodes, **128**, **136** and **138**, for shocking purposes. The housing **640** can further include a connector (not shown) having a plurality of terminals, **642**, **644**, **646**, **648**, **652**, **654**, **656**, and **658** (shown schematically and, for convenience, the names of the electrodes to which they are connected are shown next to the terminals). As such, to achieve right atrial sensing and pacing, the connector includes at least a right atrial tip terminal (A_R TIP) **642** adapted for connection to the atrial tip electrode **522**.

To achieve left atrial and ventricular sensing, pacing and shocking, the connector includes at least a left ventricular tip terminal (V_L TIP) **644**, a left atrial ring terminal (A_L RING) **646**, and a left atrial shocking terminal (A_L COIL) **648**, which are adapted for connection to the left ventricular ring electrode **526**, the left atrial tip electrode **527**, and the left atrial coil electrode **528**, respectively.

To support right ventricle sensing, pacing and shocking, the connector further includes a right ventricular tip terminal (V_R TIP) **652**, a right ventricular ring terminal (V_R RING) **654**, a right ventricular shocking terminal (R_V COIL) **656**, and an SVC shocking terminal (SVC COIL) **658**, which are adapted for connection to the right ventricular tip electrode **532**, right ventricular ring electrode **534**, the RV coil electrode **536**, and the SVC coil electrode **538**, respectively.

An atrial pulse generator **670** and a ventricular pulse generator **672** generate pacing stimulation pulses for delivery by the right atrial lead **520**, the right ventricular lead **530**, and/or the coronary sinus lead **524** via an electrode configuration switch **674**. It is understood that in order to provide stimulation therapy in each of the four chambers of the heart, the atrial and ventricular pulse generators, **670** and **672**, may include dedicated, independent pulse generators, multiplexed pulse generators, or shared pulse generators. The pulse generators, **670** and **672**, are controlled by the microcontroller **660** via appropriate control signals, **676** and **678**, respectively, to trigger or inhibit the stimulation pulses.

The microcontroller **660** further includes timing control circuitry **679** which is used to control pacing parameters (e.g., the timing of stimulation pulses) as well as to keep track of the timing of refractory periods, noise detection windows, evoked response windows, alert intervals, marker channel timing, etc., which is well known in the art. Examples of pacing parameters include, but are not limited to, atrio-ventricular delay, interventricular delay and interatrial delay.

The switch bank **674** includes a plurality of switches for connecting the desired electrodes to the appropriate I/O circuits, thereby providing complete electrode programmability. Accordingly, the switch **674**, in response to a control signal **680** from the microcontroller **660**, determines the polarity of the stimulation pulses (e.g., unipolar, bipolar, etc.) by selectively closing the appropriate combination of switches (not shown) as is known in the art.

Atrial sensing circuits **682** and ventricular sensing circuits **684** may also be selectively coupled to the right atrial lead **520**, coronary sinus lead **524**, and the right ventricular lead **530**, through the switch **674** for detecting the presence of cardiac activity in each of the four chambers of the heart. Accordingly, the atrial (ATR. SENSE) and ventricular (VTR. SENSE) sensing circuits, **682** and **684**, may include dedicated sense amplifiers, multiplexed amplifiers, or shared amplifiers. The switch **674** determines the "sensing polarity" of the cardiac signal by selectively closing the appropriate switches, as is also known in the art. In this way, the clinician may program the sensing polarity independent of the stimulation polarity.

Each sensing circuit, **682** and **684**, preferably employs one or more low power, precision amplifiers with programmable gain and/or automatic gain control, bandpass filtering, and a threshold detection circuit, as known in the art, to selectively sense the cardiac signal of interest. The automatic gain control enables the device **510** to deal effectively with the difficult problem of sensing the low amplitude signal characteristics of atrial or ventricular fibrillation. Such sensing circuits, **682** and **684**, can be used to determine cardiac performance values used in the present invention. Alternatively, an automatic sensitivity control circuit may be used to effectively deal with signals of varying amplitude.

The outputs of the atrial and ventricular sensing circuits, **682** and **684**, are connected to the microcontroller **660** which, in turn, are able to trigger or inhibit the atrial and ventricular pulse generators, **670** and **672**, respectively, in a demand fashion in response to the absence or presence of cardiac activity, in the appropriate chambers of the heart. The sensing circuits, **682** and **684**, in turn, receive control signals over signal lines, **686** and **688**, from the microcontroller **660** for purposes of measuring cardiac performance at appropriate times, and for controlling the gain, threshold, polarization charge removal circuitry (not shown), and timing of any blocking circuitry (not shown) coupled to the inputs of the sensing circuits, **682** and **686**.

One or more sensor **604** that measures a physiologic property can be located within the housing **640** of the implantable device **510**, or connected to the housing **640**.

For arrhythmia detection, the device **510** includes an arrhythmia detector **662** that utilizes the atrial and ventricular sensing circuits, **682** and **684**, to sense cardiac signals to determine whether a rhythm is physiologic or pathologic. The timing intervals between sensed events (e.g., P-waves, R-waves, and depolarization signals associated with fibrillation) can be classified by the microcontroller **660** by comparing them to a predefined rate zone limit (i.e., bradycardia, normal, low rate VT, high rate VT, and fibrillation rate zones) and various other characteristics (e.g., sudden onset, stability, physiologic sensors, and morphology, etc.) in order to assist with determining the type of remedial therapy that is needed (e.g., bradycardia pacing, anti-tachycardia pacing, cardioversion shocks or defibrillation shocks, collectively referred to as "tiered therapy"). The arrhythmia detector **662** can be implemented within the microcontroller **660**, as shown in FIG. 6. Thus, this detector **662** can be implemented by software, firmware, or combinations thereof. It is also possible that all, or portions, of the arrhythmia detector **662** can be imple-

mented using hardware. Further, it is also possible that all, or portions, of the ischemia detector **662** can be implemented separate from the microcontroller **660**.

In accordance with embodiments of the present invention, the implantable device **510** includes T-wave monitor **664**, which can monitor variability in one or more T-wave metric. Exemplary T-wave metrics, of which a variability can be calculated, include, but are not limited to: maximum amplitude of T-wave, minimum amplitude of T-wave, peak-to-peak amplitude of T-wave, location of maximum amplitude of T-wave, location of minimum amplitude of T-wave, area under T-wave, slope of T-wave, T-wave amplitude dispersion, T-wave centroid, QT interval, corrected QT interval, amplitude of ST segment, T-wave frequency content, T-wave frequency spread, and QT max-QT end. The monitor **664** can also monitor for specific changes in T-wave morphology that are known to be indicative of specific disorders, many of which were discussed above. The monitor **664** can be implemented within the microcontroller **660**, as shown in FIG. 6, and can be implemented by software, firmware, or combinations thereof. It is also possible that all, or portions, of the monitor **664** to be implemented using hardware. Further, it is also possible that all, or portions, of the monitor **664** to be implemented separate from the microcontroller **660**.

The implantable device can also include a disorder detector **665**, which can diagnose the detection of a specific change in T-wave morphology, with improved specificity, by taking into account T-wave variability and one or more propensity metric, as was described in great detail above. The detector **665** can be implemented within the microcontroller **660**, as shown in FIG. 6, and can be implemented by software, firmware, or combinations thereof. It is also possible that all, or portions, of the detector **665** to be implemented using hardware. Further, it is also possible that all, or portions, of the detector **665** to be implemented separate from the microcontroller **660**.

The implantable device can also include a medication pump **603**, which can deliver medication to a patient when episodes of specific disorder(s) are detected. Information regarding implantable medication pumps may be found in U.S. Pat. No. 4,731,051 (Fischell) and in U.S. Pat. No. 4,947,845 (Davis), both of which are incorporated by reference herein.

Still referring to FIG. 6, cardiac signals are also applied to the inputs of an analog-to-digital (A/D) data acquisition system **690**. The data acquisition system **690** is configured to acquire IEGM and/or ECG signals, convert the raw analog data into a digital signal, and store the digital signals for later processing and/or telemetric transmission to an external device **602**. The data acquisition system **690** can be coupled to the right atrial lead **320**, the coronary sinus lead **524**, and the right ventricular lead **530** through the switch **674** to sample cardiac signals across any pair of desired electrodes.

The data acquisition system **690** can be coupled to the microcontroller **660**, or other detection circuitry, for detecting an evoked response from the heart **412** in response to an applied stimulus, thereby aiding in the detection of "capture". Capture occurs when an electrical stimulus applied to the heart is of sufficient energy to depolarize the cardiac tissue, thereby causing the heart muscle to contract. The microcontroller **660** detects a depolarization signal during a window following a stimulation pulse, the presence of which indicates that capture has occurred. The microcontroller **660** enables capture detection by triggering the ventricular pulse generator **672** to generate a stimulation pulse, starting a capture detection window using the timing control circuitry **679** within the microcontroller **660**, and enabling the data acqui-

sition system **690** via control signal **692** to sample the cardiac signal that falls in the capture detection window and, based on the amplitude, determines if capture has occurred.

The implementation of capture detection circuitry and algorithms are well known. See for example, U.S. Pat. No. 4,729,376 (Decote, Jr.); U.S. Pat. No. 4,708,142 (Decote, Jr.); U.S. Pat. No. 4,686,988 (Sholder); U.S. Pat. No. 4,969,467 (Callaghan et. al.); and U.S. Pat. No. 5,350,410 (Mann et. al.), which patents are hereby incorporated herein by reference. The type of capture detection system used is not critical to the present invention.

The microcontroller **660** is further coupled to the memory **694** by a suitable data/address bus **696**, wherein the programmable operating parameters used by the microcontroller **660** are stored and modified, as required, in order to customize the operation of the implantable device **510** to suit the needs of a particular patient. The memory **694** can also be used to store information about T-wave variability, and information about diagnosed episodes relating to disorders. The memory **694** can also store information related to the patient's cardiac health and/or general wellbeing, as determined in accordance with embodiments of the present invention. Additionally, the memory **694** can be used to store propensity metrics, discussed above, which are indicative of a patient's propensity for specific disorders.

A telemetry circuit **601** can be used to wirelessly transmit such data to an external device **602**, such as a programmer, monitor, transtelephonic transceiver, or a diagnostic system analyzer. The telemetry circuit can send data indicative of T-wave variability, diagnosed episodes relating to disorders, as determined in accordance with embodiments of the present invention, to the external device **602**. Alternatively, the telemetry circuit **601** can transmit data indicative measures of T-wave morphology, and the external device **602** can determine the T-wave variability, changes in the same, and detect specific changes in T-waves that are known to be indicative of episodes relating to specific disorders. Accordingly, it can be the external device **602** that diagnoses, with improved specificity, occurrences of episodes relating to disorders that are known to affect T-wave morphology. The external device **602** can also monitor changes in a patient's general wellbeing, based on changes in the patient's T-wave variability.

The operating parameters of the implantable device **510** may be non-invasively programmed into the memory **694** through the telemetry circuit **601** in telemetric communication with an external device **602**. The telemetry circuit **601** can be activated by the microcontroller **660** by a control signal **606**. The telemetry circuit **601** advantageously allows intracardiac electrograms and status information relating to the operation of the device **510** (as contained in the microcontroller **660** or memory **694**) to be sent to the external device **602** through an established communication link **605**.

For examples of telemetry devices, see U.S. Pat. No. 4,809,697, entitled "Interactive Programming and Diagnostic System for use with Implantable Pacemaker" (Causey, III et al.); U.S. Pat. No. 4,944,299, entitled "High Speed Digital Telemetry System for Implantable Device" (Silvian); and U.S. Pat. No. 6,275,734 entitled "Efficient Generation of Sensing Signals in an Implantable Medical Device such as a Pacemaker or ICD" (McClure et al.), which patents are hereby incorporated herein by reference.

The implantable device **510** additionally includes a battery **611** which provides operating power to all of the circuits shown in FIG. 6. If the implantable device **510** also employs shocking therapy, the battery **611** should be capable of operating at low current drains for long periods of time, and then be capable of providing high-current pulses (for capacitor

charging) when the patient requires a shock pulse. The battery **611** should also have a predictable discharge characteristic so that elective replacement time can be detected.

The implantable device **510** can also include a magnet detection circuitry (not shown), coupled to the microcontroller **660**. It is the purpose of the magnet detection circuitry to detect when a magnet is placed over the implantable device **510**, which magnet may be used by a clinician to perform various test functions of the implantable device **510** and/or to signal the microcontroller **660** that the external programmer **602** is in place to receive or transmit data to the microcontroller **660** through the telemetry circuits **601**.

As further shown in FIG. 6, the device **510** is also shown as having an impedance measuring circuit **613** which is enabled by the microcontroller **660** via a control signal **614**. The known uses for an impedance measuring circuit **613** include, but are not limited to, lead impedance surveillance during the acute and chronic phases for proper lead positioning or dislodgement; detecting operable electrodes and automatically switching to an operable pair if dislodgement occurs; measuring respiration or minute ventilation; measuring thoracic impedance for determining shock thresholds and heart failure condition; detecting when the device has been implanted; measuring stroke volume; and detecting the opening of heart valves, etc. The impedance measuring circuit **613** is advantageously coupled to the switch **674** so that any desired electrode may be used. The impedance measuring circuit **613** is not critical to the present invention and is shown only for completeness.

In the case where the implantable device **510** is also intended to operate as an implantable cardioverter/defibrillator (ICD) device, it should detect the occurrence of an arrhythmia, and automatically apply an appropriate electrical shock therapy to the heart aimed at terminating the detected arrhythmia. To this end, the microcontroller **660** further controls a shocking circuit **616** by way of a control signal **618**. The shocking circuit **616** generates shocking pulses of low (up to 0.5 Joules), moderate (0.5-10 Joules), or high energy (11 to 40 Joules), as controlled by the microcontroller **660**. Such shocking pulses are applied to the patient's heart **312** through at least two shocking electrodes, and as shown in this embodiment, selected from the left atrial coil electrode **328**, the RV coil electrode **336**, and/or the SVC coil electrode **338**. As noted above, the housing **640** may act as an active electrode in combination with the RV electrode **336**, or as part of a split electrical vector using the SVC coil electrode **338** or the left atrial coil electrode **328** (i.e., using the RV electrode as a common electrode).

The above described implantable device **510** was described as an exemplary pacing device. One of ordinary skill in the art would understand that embodiments of the present invention can be used with alternative types of implantable devices. Accordingly, embodiments of the present invention should not be limited to use only with the above described device. For example, the implantable device **510** can be a simple monitoring device that does not provide any type of cardiac stimulation.

The present invention has been described above with the aid of functional building blocks illustrating the performance of specified functions and relationships thereof. The boundaries of these functional building blocks have often been arbitrarily defined herein for the convenience of the description. Alternate boundaries can be defined so long as the specified functions and relationships thereof are appropriately performed. Any such alternate boundaries are thus within the scope and spirit of the claimed invention. For example, it would be possible to combine or separate some of the steps

shown in FIGS. 2A-2C, 3 and 4. Further, it is possible to change the order of some of the steps, without substantially changing the overall events and results. For another example, it is possible to change the boundaries of some of the blocks shown in FIG. 6.

The previous description of the preferred embodiments is provided to enable any person skilled in the art to make or use the embodiments of the present invention. While the invention has been particularly shown and described with reference to preferred embodiments thereof, it will be understood by those skilled in the art that various changes in form and details may be made therein without departing from the spirit and scope of the invention.

The invention claimed is:

1. A method for monitoring for episodes relating to a disorder that is known to affect T-wave morphology, the method comprising:

- (a) using a microcontroller to monitor T-wave variability;
- (b) when the T-wave variability exceeds a corresponding threshold for a specific period of time, or a change in the T-wave variability exceeds a corresponding threshold for a specific period of time, using the microcontroller to trigger monitoring for a specific change in T-wave morphology that is known to be indicative of episodes relating to the disorder.

2. The method of claim 1, further comprising:

- (c) storing information that is indicative of the T-wave variability;
 - (d) using the microcontroller to monitor changes in the T-wave variability over time, based on the stored information; and
 - (e) using the microcontroller to interpret increases in T-wave variability as being indicative of a worsening of a patient's cardiac health, and to interpret decreases in T-wave variability as being indicative of an improvement of the patient's cardiac health.
3. The method of claim 1, further comprising:
- (c) storing information that is indicative of the T-wave variability;
 - (d) using the monitor to monitor changes in the T-wave variability over time, based on the stored information; and
 - (e) using the microcontroller to interpret increases in T-wave variability as being indicative of a worsening of a patient's general wellbeing, and to interpret decreases in T-wave variability as being indicative of an improvement of the patient's general wellbeing.

4. The method of claim 1, wherein the specific period of time is a single window of time having a duration of about 5 minutes to about one hour.

5. The method of claim 1, wherein the specific period of time comprises multiple windows of time, wherein at least a first window of time has a duration of time that is different from the duration of time of at least a second window of time.

6. The method of claim 1, wherein T-wave variability is a measure of one or more T-wave metric selected from the group consisting of:

- area under T-wave;
- slope of T-wave; and
- T-wave centroid.

7. The method of claim 1, wherein T-wave variability is a measure of the weighted average of the variability of two or more T-wave metric selected from the group consisting of:

- maximum amplitude of T-wave,
- minimum amplitude of T-wave,
- peak-to-peak amplitude of T-wave,

location of maximum amplitude of T-wave,
location of minimum amplitude of T-wave,
area under T-wave,

slope of T-wave,

T-wave amplitude dispersion,

T-wave centroid,

QT interval,

corrected QT interval,

amplitude of ST segment,

T-wave frequency content, and

T-wave frequency spread.

8. The method of claim 1, wherein T-wave variability is of variability of isochoric points of the T-wave.

9. The method of claim 1, further comprising:

- (c) using a detector to detect an episode relating to the disorder; and
- (d) using a medication pump to deliver medication to a patient when an episode relating to the disorder is detected.

10. A method for monitoring for episodes relating to a disorder that is known to affect T-wave morphology, the method comprising:

- (a) using a microcontroller to monitor T-wave variability;
- (b) when the T-wave variability exceeds a corresponding threshold for a specific period of time, or a change in the T-wave variability exceeds a corresponding threshold for a specific period of time, wherein the specific period of time comprises at least a first window having a duration of about 5 minutes to about one hour, triggering at least one of the following:
 - (b.1) an alarm; or
 - (b.2) using the microcontroller to monitor for a specific change in T-wave morphology that is known to be indicative of episodes relating to the disorder.

11. The method of claim 10, further comprising:

- (c) storing information that is indicative of the T-wave variability;
- (d) using the microcontroller to monitor changes in the T-wave variability over time, based on the stored information; and
- (e) using the microcontroller to interpret increases in T-wave variability as being indicative of a worsening of a patient's cardiac health, and to interpret decreases in T-wave variability as being indicative of an improvement of the patient's cardiac health.

12. The method of claim 10, further comprising:

- (c) storing information that is indicative of the T-wave variability;
- (d) using the microcontroller to monitor changes in the T-wave variability over time, based on the stored information; and
- (e) using the microcontroller to interpret increases in T-wave variability as being indicative of a worsening of a patient's general wellbeing, and to interpret decreases in T-wave variability as being indicative of an improvement of the patient's general wellbeing.

13. The method of claim 10, wherein T-wave variability is a measure of one or more T-wave metric selected from the group consisting of:

- area under T-wave;
- slope of T-wave; and
- T-wave centroid.

14. The method of claim 10, wherein T-wave variability is a measure of the weighted average of the variability of two or more T-wave metric selected from the group consisting of:

- maximum amplitude of T-wave,
- minimum amplitude of T-wave,

21

peak-to-peak amplitude of T-wave,
 location of maximum amplitude of T-wave,
 location of minimum amplitude of T-wave,
 area under T-wave,
 slope of T-wave,
 T-wave amplitude dispersion,
 T-wave centroid,
 QT interval,
 corrected QT interval,
 amplitude of ST segment,
 T-wave frequency content, and
 T-wave frequency spread.

15 **15.** The method of claim 10, wherein T-wave variability is of variability of isochoric points of the T-wave.

16. The method of claim 10, wherein the specific period of time further comprises at least a second window having a duration of time that is different from the duration of time of at least the first window.

17. The method of claim 10, wherein step (b) comprises using the microcontroller to monitor for a specific change in T-wave morphology that is known to be indicative of episodes relating to the disorder, and wherein the method further comprising:

- (c) using a detector to detect an episode relating to the disorder; and
- (d) using a medication pump to deliver medication to a patient when an episode relating to the disorder is detected.

18. A method for monitoring for episodes relating to a disorder that is known to affect T-wave morphology, the method comprising:

22

- (a) using a microcontroller to monitor T-wave variability, wherein T-wave variability is a measure of one or more T-wave metric selected from the group consisting of:

area under T-wave,
 slope of T-wave, and
 T-wave centroid;

- (b) when the T-wave variability exceeds a corresponding threshold for a specific period of time, or a change in the T-wave variability exceeds a corresponding threshold for a specific period of time, triggering at least one of the following

(b.1) an alarm; or

(b.2) using the microcontroller to monitor for a specific change in T-wave morphology that is known to be indicative of episodes relating to the disorder.

19. The method of claim 18, wherein the specific period of time comprises a window of time having a duration of about 5 minutes to about one hour.

20. The method of claim 18, further comprising:

- (c) storing information that is indicative of the T-wave variability;
- (d) using the microcontroller to monitor changes in the T-wave variability over time, based on the stored information; and
- (e) using the microcontroller to interpret increases in T-wave variability as being indicative of a worsening of a patient's cardiac health, and to interpret decreases in T-wave variability as being indicative of an improvement of the patient's cardiac health.

* * * * *

专利名称(译)	用于提高诊断特异性的系统和方法		
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摘要(译)

用于监测具有改善的特异性的发作的方法和装置，所述发作与已知影响T波形态的病症有关。监测T波变化。当T波可变性或其中的变化超过特定时间段的相应阈值时，可以触发监测已知指示与病症相关的发作的T波形态的特定变化。

