



US007789837B2

(12) **United States Patent**
Lehrman et al.

(10) **Patent No.:** **US 7,789,837 B2**
(45) **Date of Patent:** ***Sep. 7, 2010**

(54) **SYSTEM AND METHOD FOR TREATING OBSTRUCTIVE SLEEP APNEA**

(75) Inventors: **Michael L. Lehrman**, Washington, DC (US); **Michael E. Halleck**, Longmont, CO (US)

(73) Assignee: **iLife Systems, Inc.**, Dallas, TX (US)

(*) Notice: Subject to any disclaimer, the term of this patent is extended or adjusted under 35 U.S.C. 154(b) by 1248 days.

This patent is subject to a terminal disclaimer.

4,715,367 A	12/1987	Crossley	
4,802,485 A	2/1989	Bowers et al.	
5,058,600 A	10/1991	Schechter et al.	
5,095,900 A	3/1992	Fertig et al.	
5,123,425 A *	6/1992	Shannon et al.	128/848
5,134,995 A	8/1992	Gruenke et al.	
5,178,156 A	1/1993	Takishima et al.	
5,199,424 A *	4/1993	Sullivan et al.	128/204.18
5,265,624 A *	11/1993	Bowman	128/848
5,277,193 A	1/1994	Takishima et al.	
5,329,931 A	7/1994	Clauson et al.	

(21) Appl. No.: **11/215,360**

(Continued)

(22) Filed: **Aug. 29, 2005**

OTHER PUBLICATIONS

(65) **Prior Publication Data**

Core Textbook of Respiratory Care Practice CPR, pp. 289-292.

US 2006/0145878 A1 Jul. 6, 2006

Primary Examiner—Robert L Nasser
Assistant Examiner—Michael D'Angelo

Related U.S. Application Data

(63) Continuation of application No. 09/641,983, filed on Aug. 17, 2000, now Pat. No. 6,935,335.

(57) **ABSTRACT**

(51) **Int. Cl.**
A61B 5/08 (2006.01)

A system and method for treating obstructive sleep apnea by terminating an obstructive sleep apnea event before the cessation of breathing occurs. The system has one or more microphones capable of detecting breathing sounds within an airway of a person and that generate signals representative of the breathing sounds and send the signals to a controller. When the controller detects a signal pattern that indicates the onset of an obstructive apnea event, the controller sends an alarm signal to a stimulus generator. The stimulus generator creates a stimulus to cause the sleeping person to move in a manner to terminate the obstructive sleep apnea event before cessation of breathing occurs. The obstructive sleep apnea event is terminated without waking the sleeping person and without causing the sleeping person physiological stress associated with cessation of breathing.

(52) **U.S. Cl.** **600/538**; 600/529; 600/537; 128/200.24

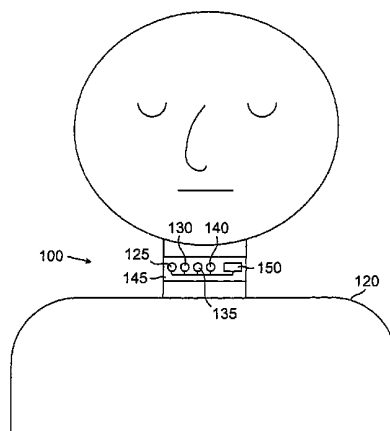
(58) **Field of Classification Search** 600/537, 600/538, 529, 533; 128/848
See application file for complete search history.

(56) **References Cited**

U.S. PATENT DOCUMENTS

4,146,885 A	3/1979	Lawson, Jr.	
4,475,559 A	10/1984	Horn	
4,595,016 A	6/1986	Fertig et al.	
4,619,270 A	10/1986	Margolis et al.	
4,630,614 A	12/1986	Atlas	
4,686,999 A *	8/1987	Snyder et al.	600/529

29 Claims, 6 Drawing Sheets



U.S. PATENT DOCUMENTS

5,385,144 A *	1/1995	Yamanishi et al.	600/330	5,844,996 A	12/1998	Enzmann et al.	
5,398,682 A	3/1995	Lynn		5,953,713 A	9/1999	Behbehani et al.	
5,605,151 A	2/1997	Lynn		5,961,447 A	10/1999	Raviv et al.	
5,652,566 A	7/1997	Lambert		6,011,477 A	1/2000	Teodorescu et al.	
5,671,733 A	9/1997	Raviv et al.		6,062,216 A	5/2000	Corn	
5,769,084 A	6/1998	Katz et al.		6,093,158 A	7/2000	Morris	
5,797,852 A	8/1998	Karakasoglu et al.		6,666,830 B1 *	12/2003	Lehrman et al.	600/586
				6,935,335 B1 *	8/2005	Lehrman et al.	128/200.24

* cited by examiner

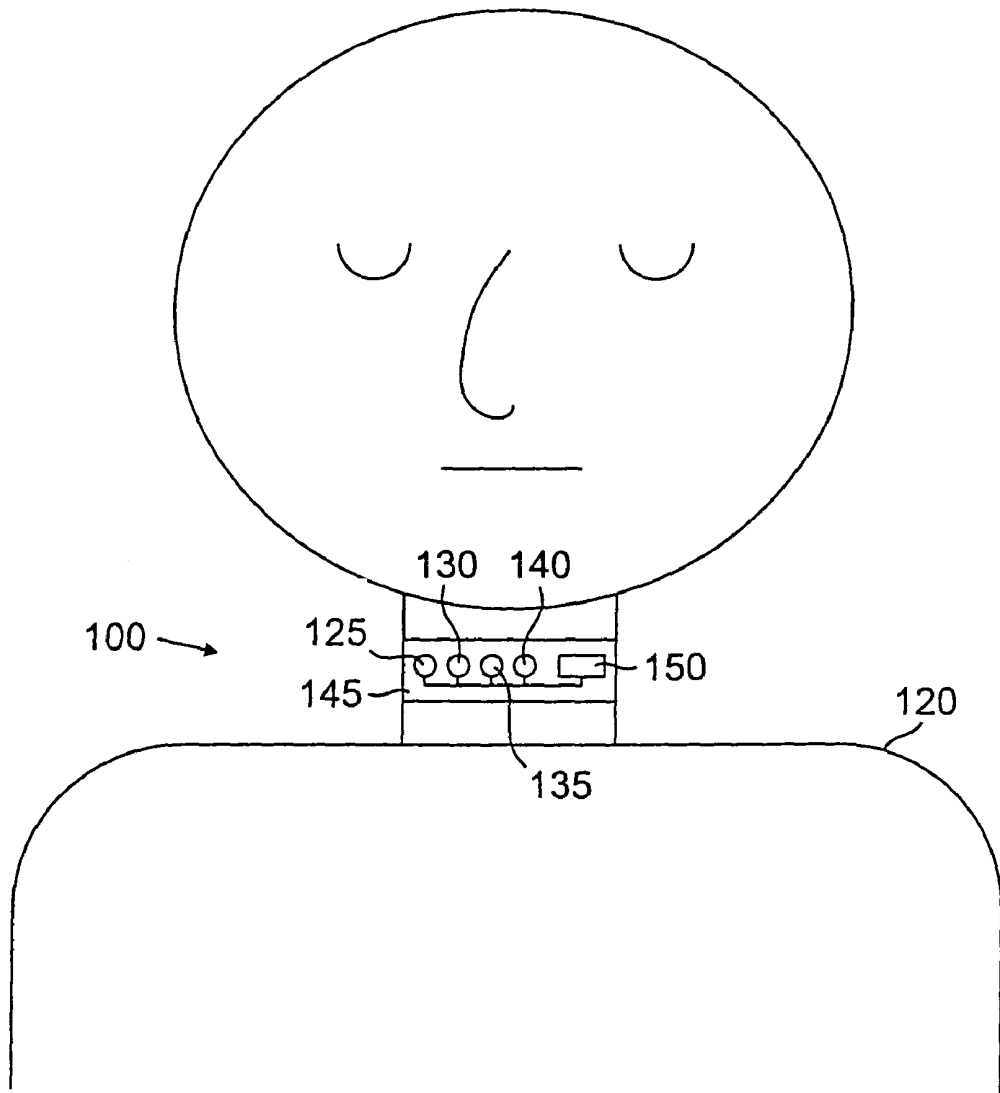


FIG. 1

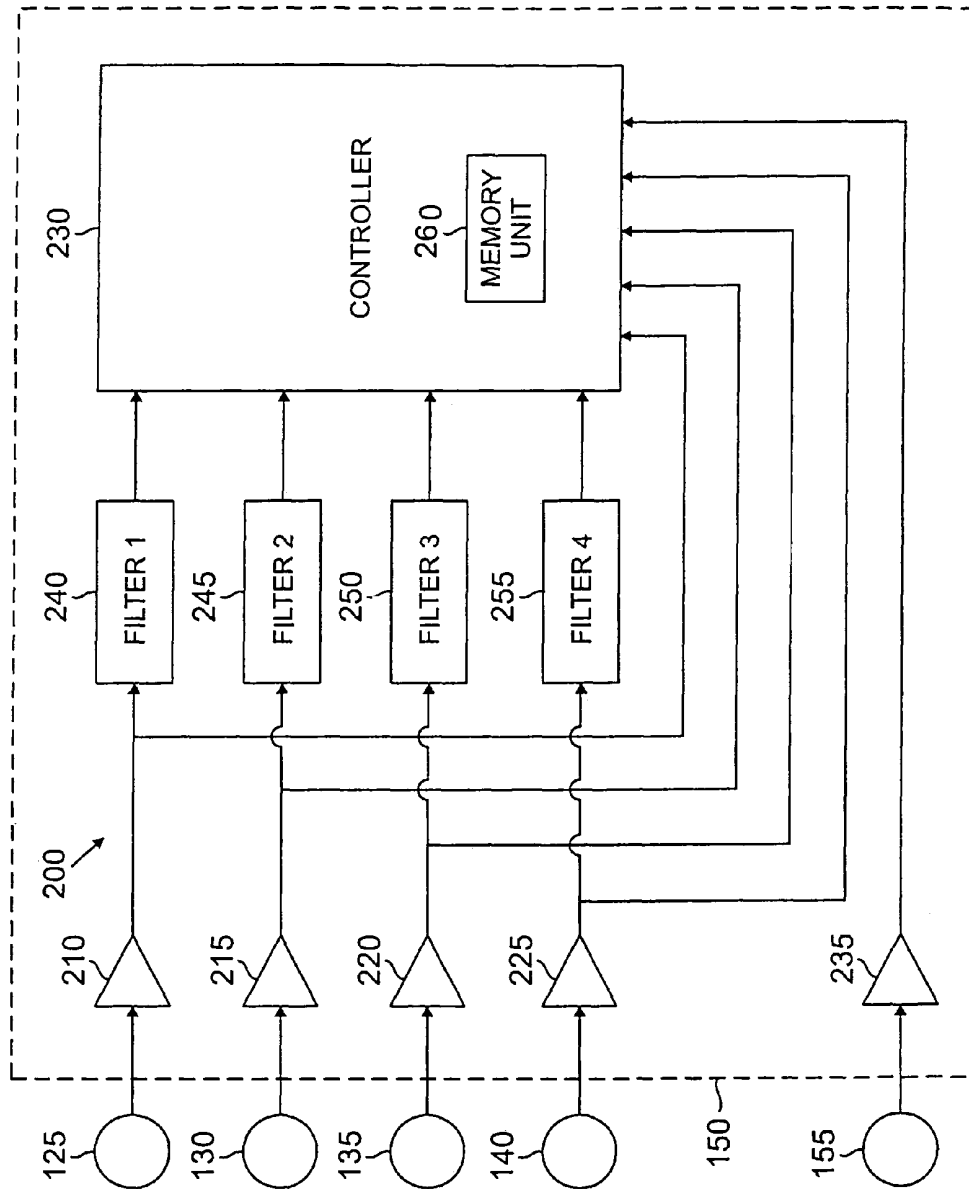


FIG. 2

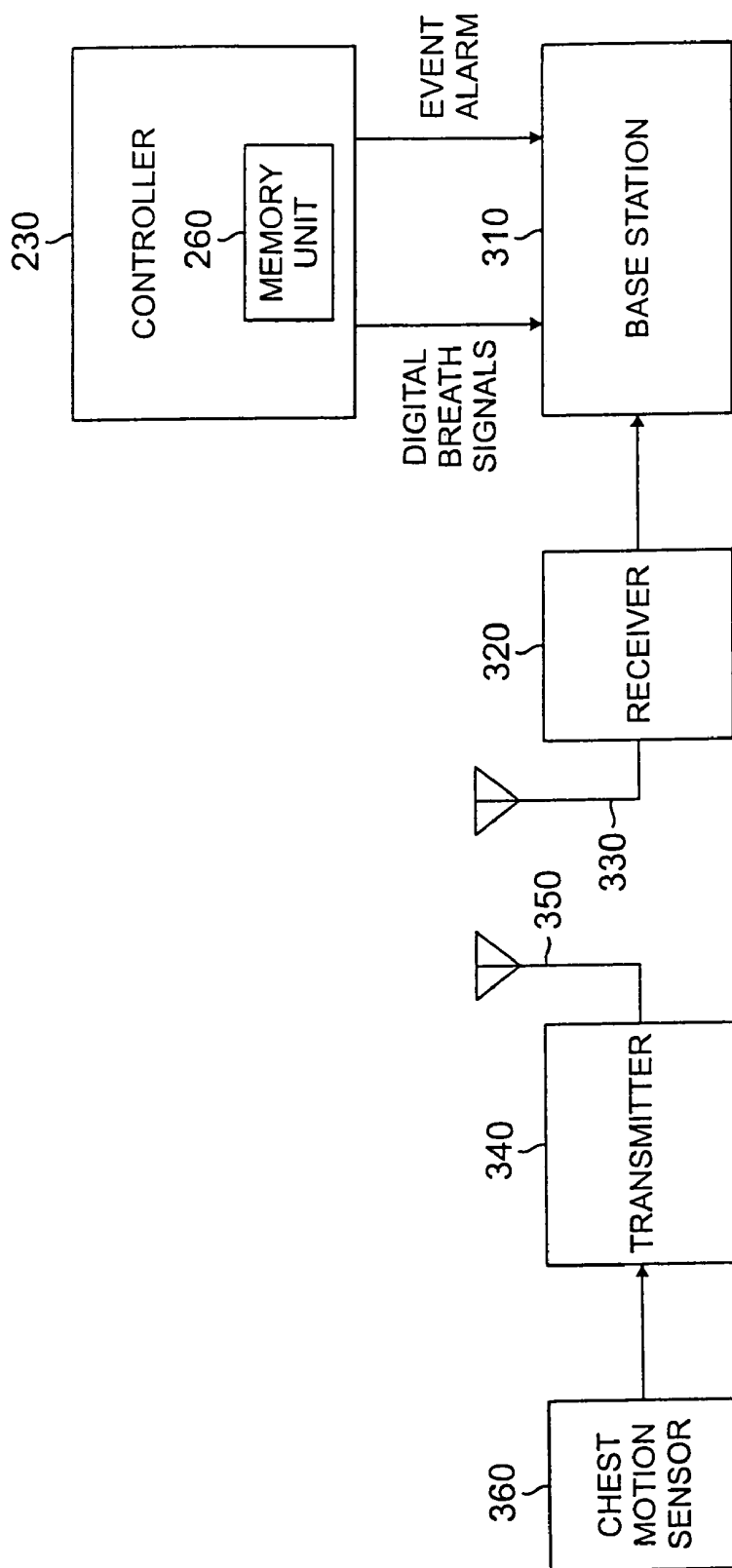


FIG. 3

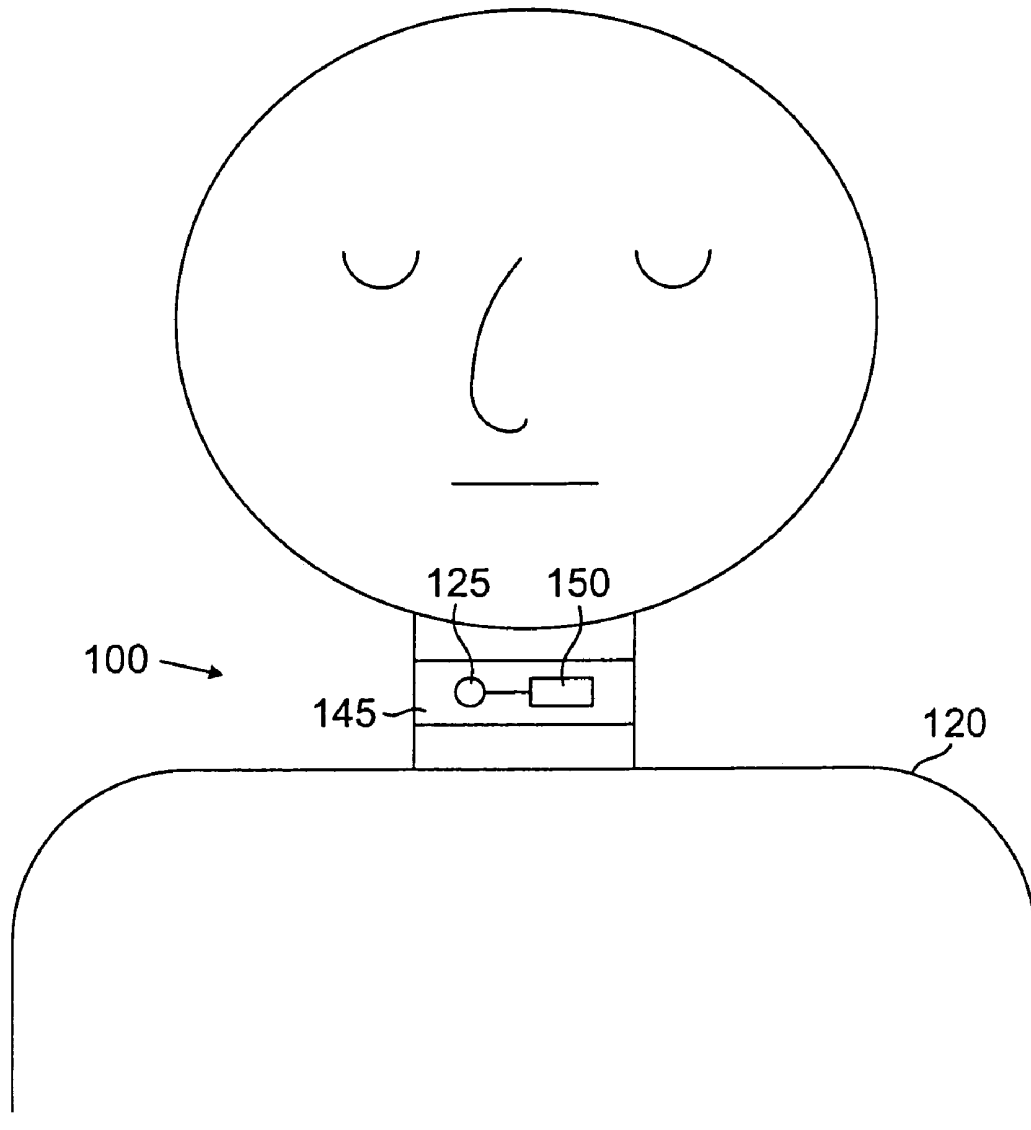


FIG. 4

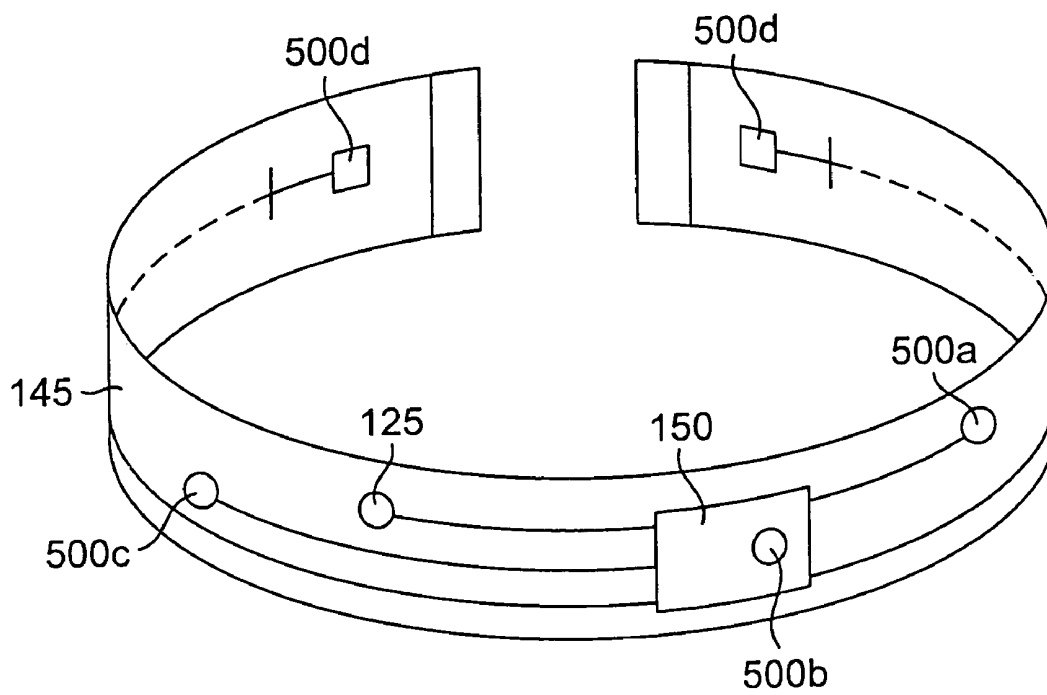


FIG. 5

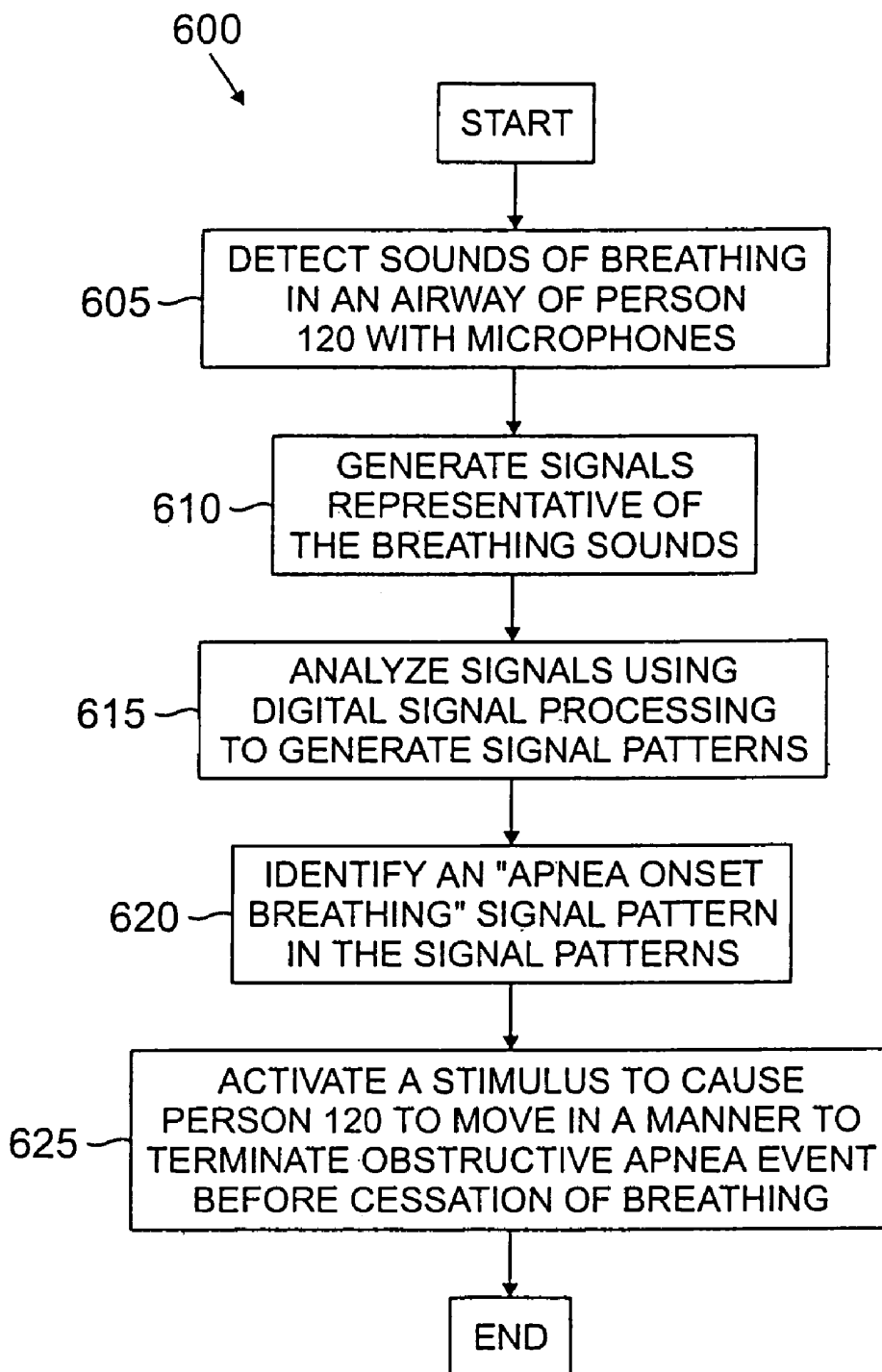


FIG. 6

SYSTEM AND METHOD FOR TREATING OBSTRUCTIVE SLEEP APNEA

This application is a continuation of prior U.S. patent application Ser. No. 09/641,983 filed on Aug. 17, 2000, which is now U.S. Pat. No. 6,935,335.

CROSS REFERENCE TO RELATED APPLICATION

The inventors of the present invention have filed a related patent application concurrently with this application entitled "System and Method for Detecting the Onset of An Obstructive Sleep Apnea Event" (application Ser. No. 09/641,982). The related patent application and the inventions disclosed therein are assigned to the assignee of the present invention and are incorporated herein by reference for all purposes as if fully set forth herein.

TECHNICAL FIELD OF THE INVENTION

The present invention is directed to a system and method for treating obstructive sleep apnea by terminating an obstructive sleep apnea event before cessation of breathing occurs.

BACKGROUND OF THE INVENTION

Apnea is the cessation of breathing. Sleep apnea is the cessation of breathing during sleep. Sleep apnea is a common sleep disorder that affects over twelve million (12,000,000) people in the United States. Persons with sleep apnea may stop and start breathing several times an hour while sleeping. Each individual episode of the cessation of breathing is referred to as a sleep apnea event.

When a person stops breathing during sleep the person's brain soon senses that oxygen levels in the blood are low and carbon dioxide levels in the blood are high. The brain then sends emergency signals to the body to cause the body to try to increase gas exchange in the lungs to increase the amount of oxygen and to decrease the amount of carbon dioxide. The body's autonomic physiological reflexes initiate survival reactions such as gasping for air, the production of enzymes to constrict arteries to increase blood pressure, and the production of enzymes to increase heart rate. The person will then usually gasp for air and thereby restore the effective gas exchange of oxygen and carbon dioxide in the lungs. This causes the sleep apnea event to end.

The brain may also cause the body's autonomic physiological reflexes to release large amounts of adrenaline in order to stir the person to gasp for air. Over a period of time repeated rushes of adrenaline in the body can have negative effects and can lead to heart damage and other medical problems.

Often the person wakes up while gasping for air. Even if the person does not become conscious while gasping for air, the body's sleep state is interrupted and the body is physiologically stressed during each sleep apnea event. Sleep apnea events can occur multiple times during a period of sleep. That is, the process of ceasing to breathe, becoming physiologically stressed, and gasping for air may be repeated numerous times during a period of sleep. Successive sleep apnea events cause a person to experience many short interrupted periods of sleep.

Interrupted periods of sleep can produce varying levels of fatigue, lack of energy, and daytime sleepiness. Other symptoms may include restless sleep, loud and sometimes heavy

snoring, morning headaches, irritability, mood changes, behavior changes, and similar emotional or physical disorders. While mild forms of sleep apnea may exist without apparent harm to the individual, severe cases may lead to such conditions as weight gain, impotency, high blood pressure, stroke, mental problems, memory loss, and even death.

There are two forms of sleep apnea. The two forms are central sleep apnea and obstructive sleep apnea. At the present time, central sleep apnea and obstructive sleep apnea are thought to originate from two different sources. Central sleep apnea appears to be linked to a malfunction of the brain that interferes with neurological signals that normally control the breathing process. Obstructive sleep apnea is caused by a blockage of the breathing airway that completely stops the flow of air to and from the lungs. A common form of obstructive sleep apnea occurs when fleshy tissue in a sleeping person's throat collapses and seals off the pharyngeal airway. A condition called mixed sleep apnea results when central sleep apnea events and obstructive sleep apnea events alternate.

Sometimes central sleep apnea directly causes death during sleep when the sleeping person completely ceasing breathing. Death results from asphyxiation due to a lack of oxygen. More frequently obstructive sleep apnea indirectly causes death because of motor vehicle crashes, job-site accidents, and similar events that are due to sleepiness caused by sleep deprivation.

Because of the variety and degree of symptoms, diagnosis of obstructive sleep apnea typically requires more than a simple analysis of symptoms. Depending upon the symptoms and severity, diagnosis may include a thorough physical exam, an examination of the mouth and throat for abnormalities, and sleep studies. Thorough sleep studies include additional tests such as electrocardiogram (ECG) tests for detecting arrhythmias, and tests for arterial blood gases to find sleep periods in which the blood oxygen level is below its normal low level.

Successful treatment for obstructive sleep apnea must ensure that a person's breathing passages remain open during sleep. The simplest treatments include weight reduction, change in body position while sleeping, avoidance of alcohol, avoidance of sedatives, and similar changes in lifestyle. When anatomical obstructions are found to be the source of obstructive sleep apnea, surgery may be required for removal of enlarged tonsils, enlarged adenoids, excess tissue at the back of the throat, and similar types of obstructions. In more extreme cases, an opening may be created in the trachea in order to bypass the obstruction that is blocking the airway during sleep.

One device for the treatment of obstructive sleep apnea is a device that pumps fresh air into a mask worn over the nose. This device provides what is known as nasal continuous positive airway pressure (CPAP). When the mask and air flow are properly adjusted, the air pressure opens the upper air passage enough to prevent snoring and obstructive sleep apnea. The disadvantages of the CPAP treatment include 1) discomfort and sleep disruption caused by the nose mask and the mechanism for connecting the mask to the air pumping device, and 2) original and on-going cost for the apparatus, and 3) inconvenience when the sleeping location changes. Some newer types of CPAP devices do not use a mask (e.g., the CPAP device disclosed in U.S. Pat. No. 6,012,455).

In addition to the more traditional treatments for obstructive sleep apnea described above, alternatives are constantly being studied and developed. Medications are being researched, but no medication has yet been developed which has proven to be effective. Mechanical devices that are inserted into the mouth while sleeping have been tried with

varying success. For instance, devices that keep the jaw or tongue in proper position are sometimes effective in cases where breathing is obstructed by a large tongue or a “set back” jaw. However, these devices have some disadvantages. They are uncomfortable to wear during sleep (which causes them to not be regularly used). Each device must have a different design for each specific type of air passage obstruction. Each device must be individually sized for each patient.

More recently, systems have been developed for the purpose of clearing upper airway passages during sleep using the electrical stimulation of nerves or muscles. In some cases, these systems require surgical implantation of sensors and associated electronics that detect when breathing has ceased and then stimulate the breathing process. Some hybrid systems have been developed that require surgical insertion of one or more sensors plus external equipment for monitoring the breathing process or moving the obstruction when breathing ceases. These systems may produce positive results but they also have associated risks due to surgery, may need replacement at later times (requiring additional surgery), and may have higher costs and lower reliability than the more traditional treatments. In addition, the hybrid systems also have the accompanying physical restrictions and accompanying disadvantages associated with connections to the external equipment.

Therefore, there is a need in the art for an improved system and method for treating obstructive sleep apnea. In particular, there is a need in the art for a system and method that does not create other types of sleep disturbing effects, does not require surgical implementation, and does not have the high costs associated with some of the types of treatments currently in use.

Prior art systems and methods are directed toward detecting and treating an obstructive sleep apnea event after the obstructive sleep apnea event has occurred. It would be very advantageous, however, to be able to detect and terminate the onset of an obstructive sleep apnea event before the obstructive sleep apnea event fully develops. That is, if the onset of an obstructive sleep apnea event can be detected before the sleeping patient actually stops breathing, steps can be taken to prevent the obstructive sleep apnea event from occurring.

Therefore, there is a need for a system and method for treating obstructive sleep apnea by terminating an obstructive sleep apnea event before the obstructive sleep apnea event fully develops. In particular, there is a need for a system and method for treating obstructive sleep apnea by terminating an obstructive sleep apnea event before cessation of breathing occurs.

SUMMARY OF THE INVENTION

The present invention is directed to a system and method for treating obstructive sleep apnea by terminating an obstructive sleep apnea event before cessation of breathing occurs.

The system of the present invention comprises one or more microphones that are capable of detecting breathing sounds within an airway of a sleeping person. The microphones generate signals that are representative of the detected breathing sounds and transfer the signals to a controller. The controller identifies at least one signal pattern that is associated with a breathing pattern of the person that occurs at the onset of an obstructive sleep apnea event. The controller may also identify at least one signal pattern that is associated with a partially occluded breathing pattern of the person. The con-

troller identifies the signal patterns by using digital signal processing techniques to analyze the signals that are representative of breathing sounds.

When the controller detects the onset of an obstructive apnea event, the controller sends a signal to a stimulus generator. The stimulus generator creates a sensory stimulus (an electric current, a sound, a flashing light, a vibrator, etc.) to cause the sleeping person to move in a manner to cause the obstructive sleep apnea event to end before cessation of breathing occurs.

It is a primary object of the present invention to provide a system and method for detecting and terminating an obstructive sleep apnea event before the obstructive sleep apnea event fully develops into cessation of breathing.

It is also an object of the present invention to provide a controller that is capable of receiving signals that are representative of breathing sounds of a person and identifying within the signals at least one signal pattern that is associated with a breathing pattern of the person that occurs at the onset of an obstructive sleep apnea event.

It is also an object of the present invention to provide a controller that is capable of receiving signals that are representative of breathing sounds of a person and identifying within the signals at least one signal pattern that is associated with a partially occluded breathing pattern of the person.

It is a further object of the present invention to provide a controller that is capable of sending a signal to activate a stimulus when the controller identifies a signal pattern that may indicate the onset of an obstructive sleep apnea event.

It is also an object of the present invention to provide a controller that is capable of identifying signal patterns by using digital signal processing techniques to analyze signals that are representative of breathing sounds.

It is a further object of the present invention to provide a method for detecting breathing sounds within an airway of a sleeping person, and generating signals that are representative of the breathing sounds, and identifying within the signals at least one signal pattern that is associated with a breathing pattern of the person that occurs at the onset of an obstructive sleep apnea event.

The foregoing has outlined rather broadly the features and technical advantages of the present invention so that those skilled in the art may better understand the detailed description of the invention that follows. Additional features and advantages of the invention will be described hereinafter that form the subject of the claims of the invention. Those skilled in the art should appreciate that they may readily use the conception and the specific embodiment disclosed as a basis for modifying or designing other structures for carrying out the same purposes of the present invention. Those skilled in the art should also realize that such equivalent constructions do not depart from the spirit and scope of the invention in its broadest form.

Before undertaking the Detailed Description, it may be advantageous to set forth definitions of certain words and phrases used throughout this patent document: the terms “include” and “comprise” and derivatives thereof mean inclusion without limitation; the term “or,” is inclusive, meaning and/or; the phrases “associated with” and “associated therewith,” as well as derivatives thereof, may mean to include, be included within, interconnect with, contain, be contained within, connect to or with, couple to or with, be communicable with, cooperate with, interleave, juxtapose, be proximate to, be bound to or with, have, have a property of, or the like; and the term “controller” means any device, system or part thereof that controls at least one operation, such a device may be implemented in hardware, firmware, or software, or

some combination of at least two of the same. It should be noted that the functionality associated with any particular controller may be centralized or distributed, whether locally or remotely. Definitions for certain words and phrases are provided throughout this patent document. Those of ordinary skill in the art should understand that in many, if not most, instances, such definitions apply to prior, as well as future uses of such defined words and phrases.

BRIEF DESCRIPTION OF THE DRAWINGS

For a more complete understanding of the present invention, and the advantages thereof, reference is now made to the following descriptions taken in conjunction with the accompanying drawings, wherein like numbers designate like objects, and in which:

FIG. 1 is diagram illustrating a plurality of microphones and a controller mounted on a collar around the neck of a person whose breathing is being monitored;

FIG. 2 is a circuit diagram illustrating the connection of the plurality of microphones in FIG. 1 to the controller of the present invention;

FIG. 3 is a circuit diagram illustrating the connection of the controller of the present invention with a base station and illustrating a communication link between a chest motion sensor and the base station;

FIG. 4 is a diagram illustrating one microphone and the controller of the present invention mounted on a collar around the neck of a person whose breathing is being monitored;

FIG. 5 is a diagram illustrating a perspective view of one embodiment of a collar on which is mounted a microphone, a controller, and a plurality of stimulus generators of the present invention; and

FIG. 6 is a flow diagram illustrating an advantageous embodiment of the method of the present invention.

DETAILED DESCRIPTION

FIGS. 1 through 6, discussed below, and the various embodiments used to describe the principles of the present invention in this patent document are by way of illustration only and should not be construed in any way to limit the scope of the invention. Those skilled in the art will understand that the principles of the present invention may be implemented in any suitably modified system for detecting and terminating an obstructive sleep apnea event.

FIG. 1 illustrates one embodiment of the present invention showing how apparatus 100 of the present invention may be attached to a person 120 who suffers from sleep apnea. Apparatus 100 may comprise either one microphone or a plurality of microphones. The embodiment of the present invention that is illustrated in FIG. 1 has four microphones 125, 130, 135, and 140. It is noted, however, that it is possible to practice the present invention using only one microphone. The embodiment of the present invention that is illustrated in FIG. 4 has only one microphone 125.

Microphones 125, 130, 135, and 140, are each capable of being acoustically associated with person 120. Microphones 125, 130, 135, and 140, are each capable of detecting sounds within a breathing airway of person 120. One type of microphone that is suitable for use in the present invention is the electret microphone. Microphones 125, 130, 135, and 140, are each attached to collar 145 and collar 145 is detachably fastened around the neck of person 120. Collar 145 may be fastened around the neck of person 120 with a velcro clasp (not shown in FIG. 1). Collar 145 is fastened around the neck

of person 120 so that microphones 125, 130, 135, and 140, are positioned adjacent a breathing airway in the neck of person 120.

Each of the microphones 125, 130, 135, and 140, is capable of generating signals representative of the sounds of breathing of person 120. When microphones 125, 130, 135, and 140, detect sounds of breathing, then each microphone generates a signal. The signals generated by each microphone are transferred via an individual microphone signal line to signal processing circuitry 200 (shown in FIG. 2) contained within housing 150.

Apparatus 100 may optionally be used in conjunction with an airflow sensor 155 (shown schematically in FIG. 2). Airflow sensor 155 is preferably attached near the nostrils of person 120. Airflow sensor 155 is capable of detecting a flow of air in and out of the nostrils of person 120 and is capable of determining the breathing rate of person 120. Airflow sensor 155 may also be located within other locations in an airway of person 120. Airflow sensors are typically capable of detecting flows of air between frequencies of one tenth Hertz (0.1 Hz) and one and one tenth Hertz (1.1 Hz).

When airflow sensor 155 detects a flow of air, then airflow sensor 155 generates an airflow detection signal. The airflow detection signal generated by airflow sensor 155 is transferred via a signal line to signal processing circuitry 200 (shown in FIG. 2) contained within housing 150. Signal processing circuitry 200 monitors the airflow detection signal of airflow sensor 155 to determine the breathing rate of person 120.

Housing 150 is mounted on collar 145 as shown in FIG. 1. Signal processing circuitry 200 within housing 150 may be connected via signal lines (not shown in FIG. 1) to base station 310 (shown in FIG. 3) located remotely from the site where person 120 is sleeping. In an alternative embodiment, signal processing circuitry 200 may transmit signal information to base station 310 through radio frequency receiver 320 (shown in FIG. 3) using a radio frequency transmitter (not shown) located within housing 150. In another alternative embodiment, signal processing circuitry 200 may transmit signal information to a network site (not shown) such as a site connected to the Internet.

FIG. 2 is a circuit diagram illustrating the connection of microphones 125, 130, 135, and 140, and optional airflow sensor 155 to controller 230 within signal processing circuitry 200. Signals from microphone 125 are transferred to amplifier 210 where the signals are amplified. Similarly, signals from microphone 130 are amplified in amplifier 215, signals from microphone 135 are amplified in amplifier 220, and signals from microphone 140 are amplified in amplifier 225. The amplified signals from amplifiers 210, 215, 220 and 225 are then transferred to controller 230.

Signals from airflow sensor 155 are transferred to amplifier 235 where the signals are amplified. The amplified signals from amplifier 235 are then transferred to controller 230.

Signals from amplifier 210 are also transferred to filter 240 (Filter 1) where the signals are filtered. In one advantageous embodiment filter 240 filters out all signals except signals having frequencies in the range of twenty Hertz (20 Hz) to one hundred Hertz (100 Hz). The filtered signals from filter 240 are then transferred to controller 230.

Similarly, signals from amplifier 215 are also transferred to filter 245 (Filter 2) where the signals are filtered. In one advantageous embodiment filter 245 filters out all signals except signals having frequencies in the range of one hundred Hertz (100 Hz) to one thousand Hertz (1,000 Hz). The filtered signals from filter 245 are then transferred to controller 230.

Similarly, signals from amplifier 220 are also transferred to filter 250 (Filter 3) where the signals are filtered. In one

advantageous embodiment filter **250** filters out all signals except signals having frequencies in the range of one thousand Hertz (1,000 Hz) to ten thousand Hertz (10,000 Hz). The filtered signals from filter **250** are then transferred to controller **230**.

Lastly, signals from amplifier **225** are also transferred to filter **255** (Filter **4**) where the signals are filtered. In one advantageous embodiment filter **250** filters out all signals except signals having frequencies in the range of ten thousand Hertz (10,000 Hz) to twenty thousand Hertz (20,000 Hz). The filtered signals from filter **255** are then transferred to controller **230**.

The numerical values given for the frequency ranges are illustrative only. It is clear that other ranges of frequency values may be used to practice the invention.

Controller **230** receives a complete set of filtered and unfiltered signals from microphones **125**, **130**, **135**, and **140**. Controller **230** may optionally receive an airflow detection signal from airflow sensor **155**. The signals from microphones **125**, **130**, **135**, and **140** will be collectively referred to as the "microphone signals." As will be more fully explained, controller **230** uses information from the microphone signals to identify a signal pattern that is associated with a breathing pattern of person **120** that occurs at the onset of an obstructive sleep apnea event.

As shown in FIG. **3**, controller **230** is coupled to base station **310**. Controller **230** continually transfers signals to base station **310** concerning the status of the breathing of person **120**. An operator of base station **310** can monitor any of the signals within controller **230**. Whenever controller **230** identifies a signal pattern that is associated with a breathing pattern of person **120** that occurs at the onset of an obstructive sleep apnea event, controller **230** initiates an obstructive sleep apnea event onset alarm and sends the obstructive sleep apnea event onset alarm to base station **310**. Similarly, whenever controller **230** receives no signals from microphones **125**, **130**, **135**, and **140**, then controller **230** assumes that person **120** is not breathing. Controller **230** then immediately initiates a "no breathing" alarm and sends the "no breathing" alarm to base station **310**.

Base station **310** is also coupled to radio frequency receiver **320** having receiver antenna **330** for receiving radio frequency transmissions from radio frequency transmitter **340** through transmitter antenna **350**. Radio frequency transmitter **340** is coupled to a chest motion sensor **360** that is coupled to the chest of person **120**. Chest motion sensor **360** senses the rhythmical motion of the chest of person **120** during breathing. In this manner, radio frequency transmitter **340** continually transfers signals to base station **310** concerning the status of the chest motion of person **120**.

Controller **230** comprises software for analyzing the microphone signals. The software in controller **230** utilizes digital signal processing techniques for finding the frequency domain components of each microphone signal. The digital signal processing techniques used by controller **230** may be of any type including, without limitation, Fast Fourier Transform techniques. Controller **230** also comprises memory unit **260** that is capable of storing 1) digital signal processing analysis software for analyzing the microphone signals, and 2) signal patterns that result from the digital signal processing analysis of the microphone signals, and 3) software for comparing signal patterns.

Controller **230** is capable of identifying and storing signal patterns from the microphone signals. For example, when person **120** is breathing normally, controller **230** receives microphone signals that indicate normal breathing. The signal pattern that results from the digital signal processing

analysis of the "normal breathing" microphone signals is stored in memory unit **260** as a "normal breathing" signal pattern. Controller **230** is capable of recalling the "normal breathing" signal pattern from memory unit **260** in order to compare other signal patterns with the "normal breathing" signal pattern.

A person who suffers from sleep apnea will often exhibit a breathing pattern in which the flow of air through an airway is partially occluded. This means that at least one portion of the airway is not fully open. Although air flows through the airway, the air is constricted as it passes through the partially occluded airway. The sound of air as it passes through a partially occluded airway differs from the sound of air as it passes through a fully open airway. That is, the sound of partially occluded breathing has different sound characteristics than the sound of normal breathing.

When person **120** begins to exhibit a breathing pattern in which the flow of air is partially occluded, then controller **230** receives microphone signals that are indicative of partially occluded breathing. The signal pattern that results from the digital signal processing analysis of the "partially occluded breathing" microphone signals is stored in memory unit **260** as a "partially occluded breathing" signal pattern. Controller **230** is capable of recalling the "partially occluded breathing" signal pattern from memory unit **260** in order to compare other signal patterns with the "partially occluded breathing" signal pattern.

While person **120** is breathing, controller **230** is capable of monitoring the microphone signals that are representative of the breathing sounds. Controller **230** is also capable of obtaining the signal patterns that result from the digital signal processing analysis of the microphone signals. Controller **230** is also capable of comparing the current signal patterns with the "partially occluded breathing" signal pattern. When controller **230** determines that a current signal pattern is substantially the same as the "partially occluded breathing" signal pattern, then controller **230** sends an alarm signal to base station **310**. The alarm signal indicates that at least one signal pattern has been identified that is associated with a partially occluded breathing pattern.

As will be more fully explained below, controller **230** is also capable of sending a signal to at least one stimulus generator **500** (shown in FIG. **5**) when controller **230** detects a "partially occluded breathing" signal pattern. Stimulus generator **500** creates a stimulus to cause person **120** to move in a manner that terminates the partial occlusion of the breathing and restores normal breathing.

At the onset of an obstructive sleep apnea event, a person may exhibit a breathing pattern in which the flow of air through an airway differs from normal breathing. In such cases, the sound of air as it passes through the airway at the onset of an obstructive sleep apnea event differs from the sound of air as it passes through a fully open airway. That is, the sound of breathing at the onset of an obstructive sleep apnea event has different sound characteristics than the sound of normal breathing.

When person **120** begins to exhibit a breathing pattern associated with the onset of an obstructive sleep apnea event, then controller **230** receives microphone signals that are indicative of "apnea onset breathing." The signal pattern that results from the digital signal processing analysis of the "apnea onset breathing" microphone signals is stored in memory unit **260** as an "apnea onset breathing" signal pattern. Controller **230** is capable of recalling the "apnea onset breathing" signal pattern from memory unit **260** in order to compare other signal patterns with the "apnea onset breathing" signal pattern.

While person 120 is breathing, controller 230 is capable of monitoring the microphone signals that are representative of the breathing sounds. Controller 230 is also capable of obtaining the signal patterns that result from the digital signal processing analysis of the microphone signals. Controller 230 is also capable of comparing the current signal patterns with the “apnea onset breathing” signal pattern. When controller 230 determines that a current signal pattern is substantially the same as the “apnea onset breathing” signal pattern, then controller 230 sends an alarm signal to base station 310. The alarm signal indicates that at least one signal pattern has been identified that is associated with a breathing pattern that occurs at the onset of an obstructive sleep apnea event.

After controller 230 signals that person 120 is exhibiting a breathing pattern that is associated with the onset of an obstructive sleep apnea event, steps may be taken to stimulate the body of person 120 in a manner that will terminate the obstructive sleep apnea event (before cessation of breathing occurs) without causing person 120 to wake up.

This may be accomplished by controller 230 sending an alarm signal to at least one stimulus generator 500 (shown in FIG. 5). In response to the alarm signal, stimulus generator 500 creates a stimulus to cause person 120 to move in a manner that terminates the obstructive apnea event before the cessation of breathing occurs. Stimulus generator 500 may comprise, without limitation, a sound generator 500a, or a light source 500b, or a vibrator 500c, or an electrical current source 500d (e.g., battery powered electrodes 500d) for sending a mild electric current into the neck muscles of person 120.

FIG. 5 shows how stimulus generators 500a, 500b, 500c, and 500d may be mounted on collar 145. The embodiment shown in FIG. 5 comprises housing 150 and one microphone 125. Controller 230 within housing 150 can send an alarm signal to sound generator 500a to cause sound generator 500a to create an audible sound. Similarly, controller 230 within housing 150 can send an alarm signal to light source 500b (shown mounted on housing 150) to cause light source 500b to turn on a light. Similarly, controller 230 within housing 150 can send an alarm signal to cause vibrator 500c to vibrate. Similarly, controller 230 within housing 150 can send an alarm signal to cause electrical current source 500d to generate a mild electric current. The electrodes 500d representing electrical current source 500d are powered by a battery (not shown in FIG. 5). Controller 230 within housing 150 may activate stimulus generators 500a, 500b, 500c, and 500d individually or in any combination.

The stimuli generated by stimulus generators 500a, 500b, 500c, and 500d, are designed to be at a low level of intensity so that person 120 does not wake up when the stimuli are activated. While person 120 is sleeping, person 120 is capable of subconsciously perceiving the activation of the low intensity stimuli. Person 120 may be trained to subconsciously respond to one or more of the stimuli by inclining his or her head backwards. The backward movement of the head opens the airways of person 120 and terminates the obstructive apnea event. When controller 230 senses the presence of normal breathing, then controller 230 sends a signal to stimulus generators 500a, 500b, 500c, and 500d to cease generating the stimuli. In this manner, an obstructive apnea event can be terminated before cessation of breathing occurs without waking up the person who is experiencing the obstructive apnea event.

As previously described, controller 230 may receive an airflow detection signal from airflow sensor 155. Controller 230 is capable of determining from the airflow detection signal when person 120 is inhaling and exhaling. Controller

230 is also capable of determining from the microphone signals when person 120 is inhaling and exhaling. In an alternate advantageous embodiment of the present invention, controller 230 shuts down and ceases monitoring the signal patterns 1) during exhalation, or 2) during inhalation. By operating only during one half of the respiratory cycle, controller 230 uses only one half of the power that would otherwise be required.

If the onset of obstructive sleep apnea fully develops, then cessation of breathing will occur. When person 120 ceases to breathe, then microphones 125, 130, 135, and 140, detect no breathing sounds. When controller 230 receives signals that indicate that a “no breathing” condition has occurred, then controller 230 sends a “no breathing” alarm signal as previously described.

After breathing ceases, a short period of time will pass before the brain will begin to detect and respond to the resulting lower levels of oxygen in the blood. This period of time will normally last several tens of seconds. During this time period controller 230 may send a “no breathing” alarm signal to at least one stimulus generator 500 as previously described. In response to the alarm signal, stimulus generator 500 creates a stimulus to cause person 120 to move in a manner that terminates the obstructive apnea event. In this manner, the apparatus and method of the present invention is capable of causing an obstructive apnea event to be terminated after breathing has ceased but before the physiological stress associated with cessation of breathing has become severe.

FIG. 6 illustrates a flow chart 600 depicting the operation of one advantageous embodiment of the present invention. First, microphones 125, 130, 135, and 140, detect sounds of breathing in the airways of person 120 (process step 605) and generate signals that are representative of the breathing sounds (process step 610). Controller 230 then analyzes the signals using digital signal processing software (e.g., Fast Fourier Transform analysis software) to generate signal patterns that are representative of the signals (process step 615).

Controller 230 monitors the signal patterns to identify a signal pattern that is associated with a breathing pattern that occurs at the onset of an obstructive sleep apnea event (process step 620). Controller 230 then sends a signal to activate a stimulus (electrical current, sound, vibration, light flash, etc.) to cause person 120 to move in a manner that causes the airways of person 120 to open and terminate the obstructive apnea event before cessation of breathing occurs (process step 625).

Although the present invention has been described in detail, those skilled in the art should understand that they can make various changes, substitutions and alterations herein without departing from the spirit and scope of the invention in its broadest form.

What is claimed is:

1. An apparatus for treating an obstructive sleep apnea event before the cessation of breathing occurs, wherein the apparatus comprises:

at least one microphone capable of being acoustically associated with a person, said microphone capable of detecting breathing of said person and capable of generating signals representative of said breathing;

a controller associated with said at least one microphone wherein said controller receives said signals and identifies within said signals at least one signal pattern that is associated with a breathing pattern of said person that occurs at the onset of an obstructive sleep apnea event; and

a stimulus generator associated with said controller, wherein said stimulus generator receives from said con-

troller at least one signal pattern that is associated with a breathing pattern of said persons that occurs at the onset of an obstructive sleep apnea event, and in response thereto, creates a stimulus to cause said person's head to move backward to end said obstructive sleep apnea event before cessation of breathing occurs.

2. An apparatus as set forth in claim 1 wherein said stimulus generator comprises an electrical current source placed adjacent to said person's neck.

3. An apparatus as set forth in claim 1 wherein said stimulus generator comprises a vibrator and a sound generator placed adjacent to said person's neck.

4. An apparatus as set forth in claim 1 wherein said stimulus generator comprises a vibrator and an electrical current source placed adjacent to said person's neck.

5. An apparatus as set forth in claim 1 further comprising a base station coupled to said controller wherein said controller is capable of sending an alarm signal to said base station to indicate that at least one signal pattern has been identified that is associated with a breathing pattern of said person that occurs at the onset of an obstructive sleep apnea event before cessation of breathing occurs.

6. An apparatus as set forth in claim 1 further comprising at least one filter coupled between said at least one microphone and said controller, wherein said at least one filter is capable of filtering said signals from said at least one microphone to create filtered signals representative of said breathing sounds, and wherein said controller is capable of identifying within said filtered signals at least one signal pattern that is associated with a breathing pattern of said person that occurs at the onset of an obstructive sleep apnea event.

7. The apparatus as set forth in claim 1 further comprising an airflow sensor capable of detecting a flow of air within an airway of said person and capable of generating an airflow detection signal that is representative of the presence of said flow of air; and wherein said controller is coupled to said airflow sensor and is capable of receiving said airflow detection signal from said airflow sensor to obtain information concerning the breathing of said person.

8. The apparatus as set forth in claim 1 wherein said controller comprises software capable of analyzing said signals to identify within said signals at least one signal pattern that is associated with a breathing pattern of said person that occurs at the onset of an obstructive sleep apnea event.

9. The apparatus as set forth in claim 8 wherein said software analyzes said signals using Fast Fourier Transform analysis.

10. The apparatus as set forth in claim 1 wherein said controller operates only during one half of the respiration cycle.

11. An apparatus for treating an obstructive sleep apnea event before the cessation of breathing occurs, wherein the apparatus comprises:

at least one microphone capable of being acoustically associated with a person, wherein said microphone detects breathing of said person and generates signals representative of said breathing;

a controller associated with said at least one microphone, wherein said controller receives said signals and identifies within said signals at least one signal pattern that is associated with a partially occluded breathing pattern of said person; and

a stimulus generator associated with said controller, wherein said stimulus generator receives from said controller at least one signal pattern that is associated with a partially occluded breathing pattern of said person, and in response thereto, creates a stimulus to cause said

person's head to move backward to end partially occluded breathing of said person and restore normal breathing before cessation of breathing occurs.

12. An apparatus as set forth in claim 11 wherein said stimulus generator comprises an electrical current source placed adjacent to said person's neck.

13. An apparatus as set forth in claim 11 wherein said stimulus generator comprises a vibrator and a sound generator placed adjacent to said person's neck.

14. An apparatus as set forth in claim 11 wherein said stimulus generator comprises a vibrator and an electrical current source placed adjacent to said person's neck.

15. An apparatus as set forth in claim 11 further comprising a base station coupled to said controller wherein said controller is capable of sending an alarm signal to said base station to indicate that at least one signal pattern has been identified that is associated with a partially occluded breathing pattern of said person.

16. An apparatus as set forth in claim 11 further comprising at least one filter coupled between said microphone and said controller, wherein said at least one filter is capable of filtering said signals from said at least one microphone to create filtered signals representative of said breathing sounds, and wherein said controller is capable of identifying within said filtered signals at least one signal pattern that is associated with a partially occluded breathing pattern of said person.

17. An apparatus as set forth in claim 11 further comprising an airflow sensor capable of detecting a flow of air within an airway of said person and capable of generating an airflow detection signal that is representative of the presence of said flow of air; and wherein said controller is coupled to said airflow sensor and is capable of receiving said airflow detection signal from said airflow sensor to obtain information concerning the breathing of said person.

18. An apparatus as set forth in claim 11 wherein said controller comprises software capable of analyzing said signals to identify within said signals at least one signal pattern that is associated with a partially occluded breathing pattern of said person.

19. An apparatus as set forth in claim 11 wherein said software analyzes said signals using Fast Fourier Transform analysis.

20. An apparatus as set forth in claim 11 wherein said controller operates only during one half of the respiration cycle.

21. A method for treating an obstructive sleep apnea event before the cessation of breathing occurs, comprising the steps of:

detecting, at a microphone, breathing of a person;
generating, at the microphone, signals representative of said breathing;

identifying, at a controller, within said signals at least one signal pattern that occurs at the onset of an obstructive sleep apnea event; and

creating, at a stimulus generator, a stimulus to cause said person's head to move backwards in a manner that causes said obstructive sleep apnea event to end.

22. The method as set forth in claim 21 wherein said step of creating a stimulus to cause said person's head to move backwards in a manner that causes said obstructive sleep apnea event to end comprises the steps of: activating a vibrator placed adjacent to said person's neck muscles and generating a sound with a sound generator placed adjacent to said person's neck muscles.

23. The method as set forth in claim 21 wherein said step of creating a stimulus to cause person's head to move backwards in a manner that causes said obstructive sleep apnea event to

13

end comprises the steps of: activating a vibrator placed adjacent to said person's neck muscles and generating an electrical current through the neck muscles of said person.

24. The method as set forth in claim 21 wherein said step of creating a stimulus to cause said person's head to move backwards in a manner that causes said obstructive sleep apnea event to end comprises the step of generating an electrical current through the neck muscles of said person.

25. The method as set forth in claim 21 further comprising the steps of:

filtering said signals representative of said breathing to create filtered signals representative of said breathing; and

identifying within said filtered signals at least one signal pattern that is associated with a breathing pattern of said person that occurs at the onset of an obstructive sleep apnea event.

26. The method as set forth in claim 21 further comprising the steps of:

recording said at least one signal pattern that is associated with a breathing pattern of said person that occurs at the onset of an obstructive sleep apnea event;

monitoring said signals representative of said breathing as said person breathes;

comparing said signals representative of said breathing with said recorded at least one signal pattern that is associated with a breathing pattern of said person that occurs at the onset of an obstructive sleep apnea event; and

identifying within said signals a signal pattern that is substantially the same as said recorded at least one signal pattern that is associated with a breathing pattern of said person that occurs at the onset of an obstructive sleep apnea event.

27. The method as set forth in claim 21 wherein the step of detecting breathing of said person comprises:

detecting breathing within an airway of said person only during one half of the respiration cycle.

28. A method for treating an obstructive sleep apnea event before the cessation of breathing occurs comprising the steps of:

detecting, at a microphone, breathing of a person;

generating, at the microphone, signals representative of said breathing;

14

identifying, at a controller, within said signals at least one signal pattern that is associated with a partially occluded breathing pattern of said person;

recording, at the controller, said at least one signal pattern that is associated with a partially occluded breathing pattern of said person;

monitoring, at the controller, said signals representative of said breathing as said person breathes;

comparing, at the controller, said signals representative of said breathing with said recorded at least one signal pattern that is associated with a partially occluded breathing pattern of said person;

identifying, at the controller, within said signals a signal pattern that is substantially the same as said recorded at least one signal pattern that is associated with a partially occluded breathing pattern of said person; and

creating, at a stimulus generator, a stimulus to cause said person's head to move backward to end a partially occluded breathing pattern of said person and restore normal breathing before cessation of breathing occurs.

29. A method for treating an obstructive sleep apnea event before the cessation of breathing occurs comprising the steps of:

detecting, at a microphone, breathing of a person;

generating, at the microphone, signals representative of said breathing;

identifying, at a controller, within said signals at least one signal pattern that is associated with a normal breathing pattern of said person;

recording, at the controller, said at least one signal pattern that is associated with a normal breathing pattern of said person;

monitoring, at the controller, said signals representative of said breathing as said person breathes;

comparing, at the controller, said signals representative of said breathing with said recorded at least one signal pattern that is associated with a normal breathing pattern of said person;

identifying, at the controller, within said signals a signal pattern that is substantially different from said recorded at least one signal pattern that is associated with a normal breathing pattern of said person; and

creating, at the controller, a stimulus to cause said person's head to move backward to restore normal breathing before cessation of breathing occurs.

* * * * *

专利名称(译)	治疗阻塞性睡眠呼吸暂停的系统和方法		
公开(公告)号	US7789837	公开(公告)日	2010-09-07
申请号	US11/215360	申请日	2005-08-29
[标]申请(专利权)人(译)	ILIFE系统公司		
申请(专利权)人(译)	ILIFE系统公司.		
当前申请(专利权)人(译)	ILIFE系统公司.		
[标]发明人	LEHRMAN MICHAEL L HALLECK MICHAEL E		
发明人	LEHRMAN, MICHAEL L. HALLECK, MICHAEL E.		
IPC分类号	A61B5/08 A61B5/00 A61B7/00 A61M16/00 A61N1/36		
CPC分类号	A61B5/0002 A61B5/4818 A61B5/6822 A61B7/003 A61M16/00 A61M16/0051 A61N1/3601 A61M16/0069 A61M2205/3375 A61M2205/581 A61M2205/582 A61M2205/583 A61M2205/587 A61M16/024		
助理审查员(译)	德安杰洛, MICHAEL		
其他公开文献	US20060145878A1		
外部链接	Espacenet USPTO		

摘要(译)

通过在呼吸停止之前终止阻塞性睡眠呼吸暂停事件来治疗阻塞性睡眠呼吸暂停的系统和方法。该系统具有一个或多个能够检测人的气道内的呼吸声并且产生代表呼吸声的信号并将信号发送到控制器的麦克风。当控制器检测到指示阻塞性呼吸暂停事件发作的信号模式时，控制器向刺激发生器发送警报信号。刺激发生器产生刺激以使睡眠者在停止呼吸发生之前终止阻塞性睡眠呼吸暂停事件的方式移动。阻塞性睡眠呼吸暂停事件终止而不会使睡眠者醒来并且不会导致睡眠者与停止呼吸相关的生理压力。

