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Ince et al.

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(54) **PULSED LIGHTING IMAGING SYSTEMS
AND METHODS**

USPC 600/310, 316, 322, 365, 473, 476, 323;
356/364, 367, 369, 477, 479
See application file for complete search history.

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(*) Notice: Subject to any disclaimer, the term of this
patent is extended or adjusted under 35
U.S.C. 154(b) by 133 days.

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Related U.S. Application Data

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(51) **Int. Cl.**
A61B 6/00 (2006.01)
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Primary Examiner — Katherine Fernandez
(74) *Attorney, Agent, or Firm* — Anderson IP, Inc.

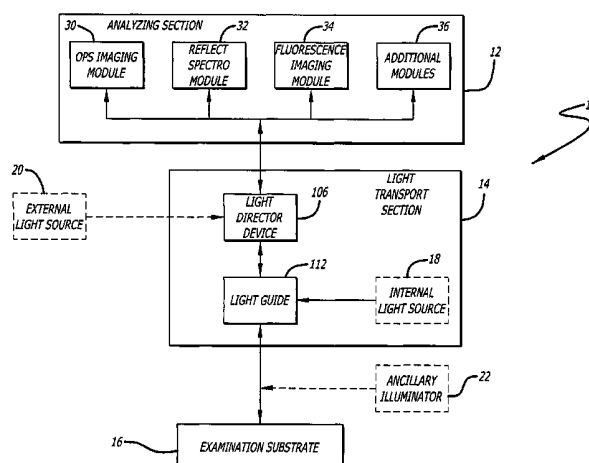
(52) **U.S. Cl.**
CPC **A61B 5/0261** (2013.01); **A61B 1/00186**
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(57) **ABSTRACT**

Systems and methods for monitoring patients utilizing reflec-
tance avoidance as well as other imaging modalities. Informa-
tion regarding perfusion, oxygen saturation and oxygen
availability, as well as others may be obtained. System
embodiments may include a light source, a light transport
body configured to project light from the light source to an
examination substrate and transmit light reflected by the
examination substrate, and an analysis section in optical com-
munication with the light transport body. The light source
may be pulsed in order to improve the quality of video images
produced by the systems.

(58) **Field of Classification Search**
CPC H01G 9/012; H01G 9/15; H01G 9/10;
H01G 2/065; H01G 9/0029; H01G 9/008;
H01G 9/04; H01G 9/042; H01G 9/052;
H01G 9/08; Y10T 29/417; A61B 1/00186;
A61B 1/042; A61B 1/043; A61B 1/06;
A61B 1/0646; A61B 1/0684; A61B 5/0059;
A61B 5/0261; A61B 5/14556; A61B 5/412;
A61B 1/0607; A61B 1/0638; G02B 21/084;
G02B 21/365; H05K 1/182

30 Claims, 17 Drawing Sheets



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A61B 5/026 (2006.01)
A61B 1/04 (2006.01)
A61B 1/06 (2006.01)
A61B 5/1455 (2006.01)
G02B 21/08 (2006.01)
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CPC **A61B 1/043** (2013.01); **A61B 1/06**
 (2013.01); **A61B 1/0607** (2013.01); **A61B**
1/0646 (2013.01); **A61B 1/0684** (2013.01);
A61B 5/14556 (2013.01); **A61B 5/412**
 (2013.01); **G02B 21/084** (2013.01); **G02B**
21/365 (2013.01); **A61B 1/0638** (2013.01);
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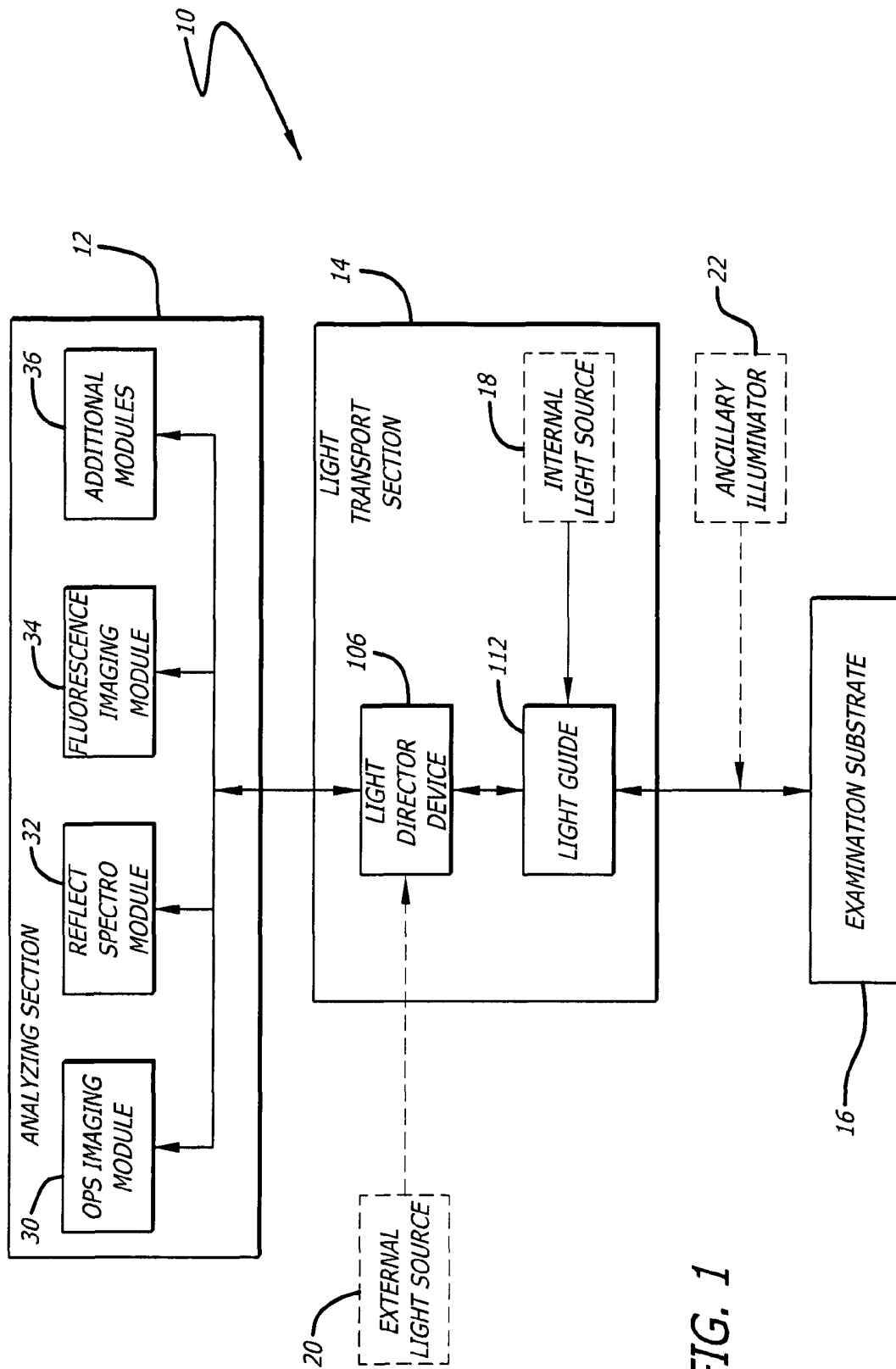
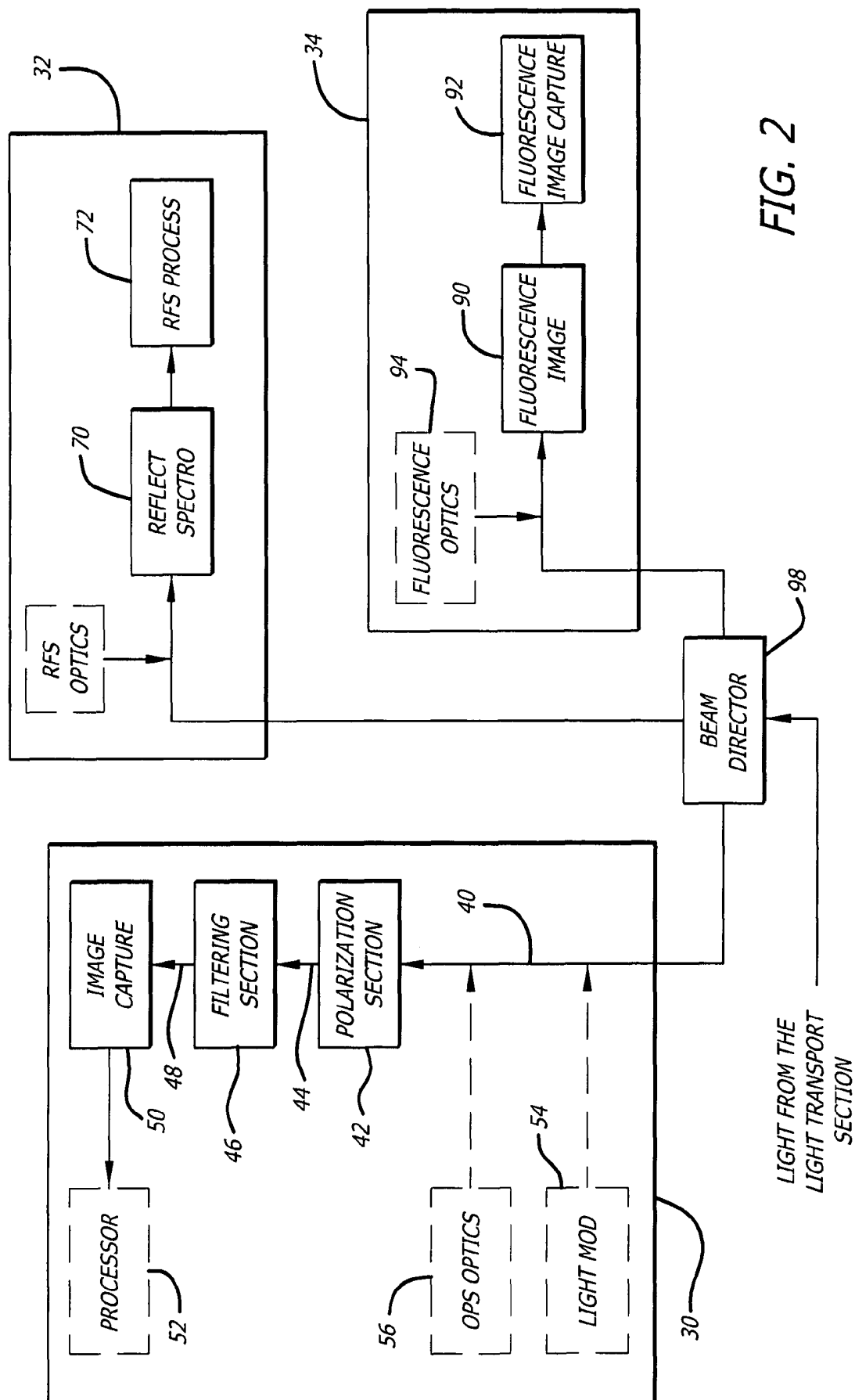


FIG. 1



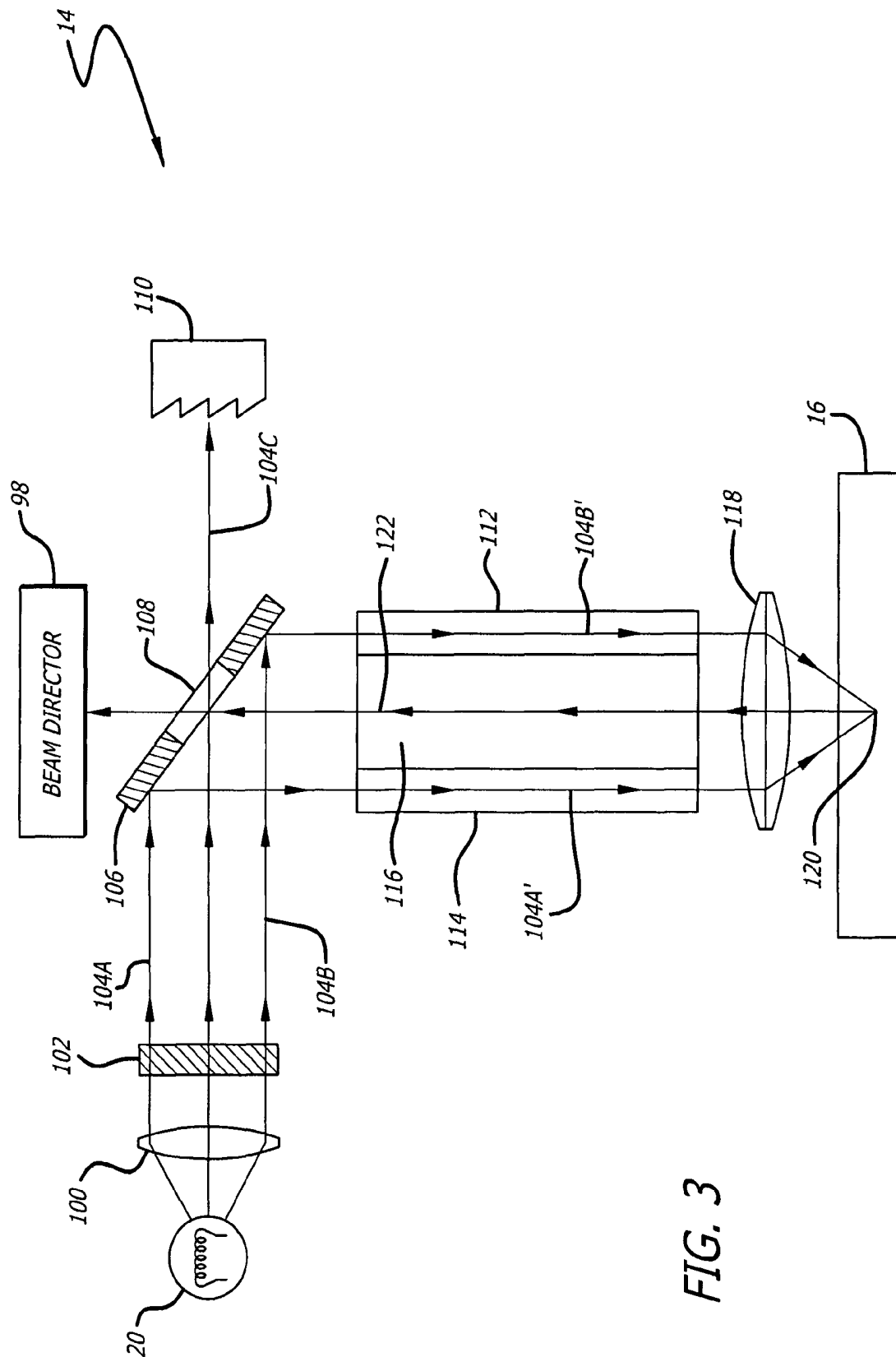
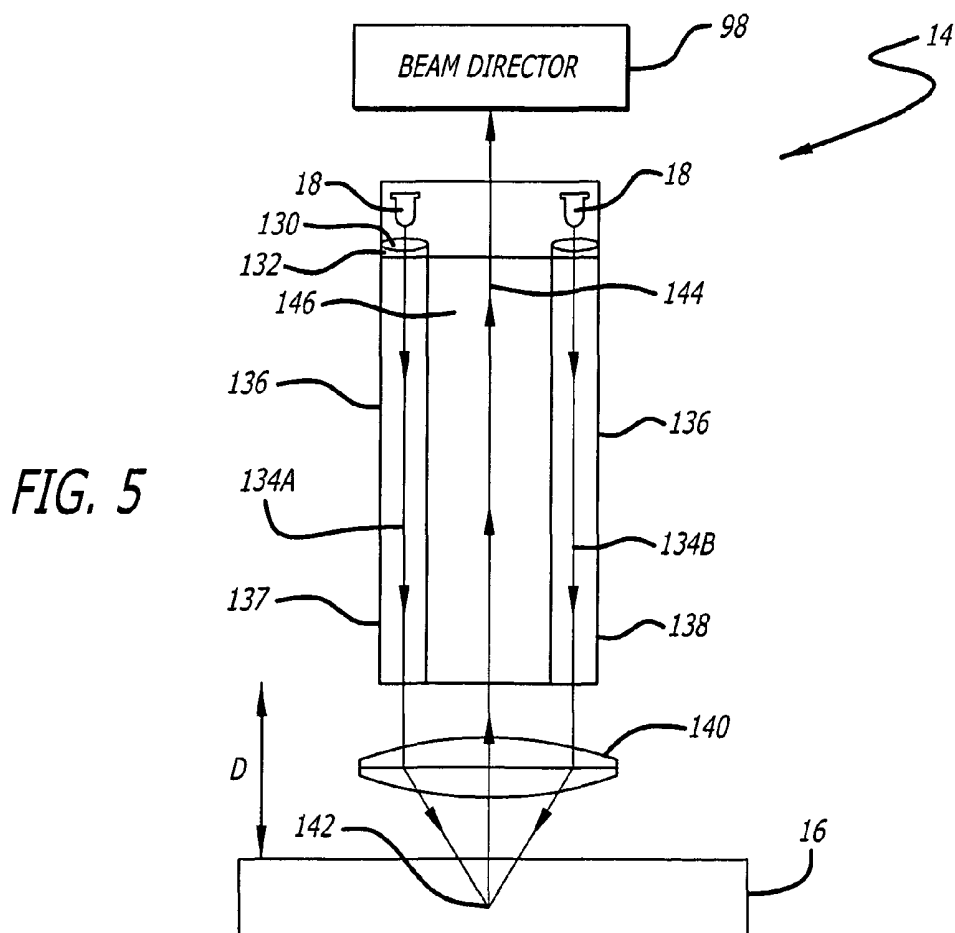
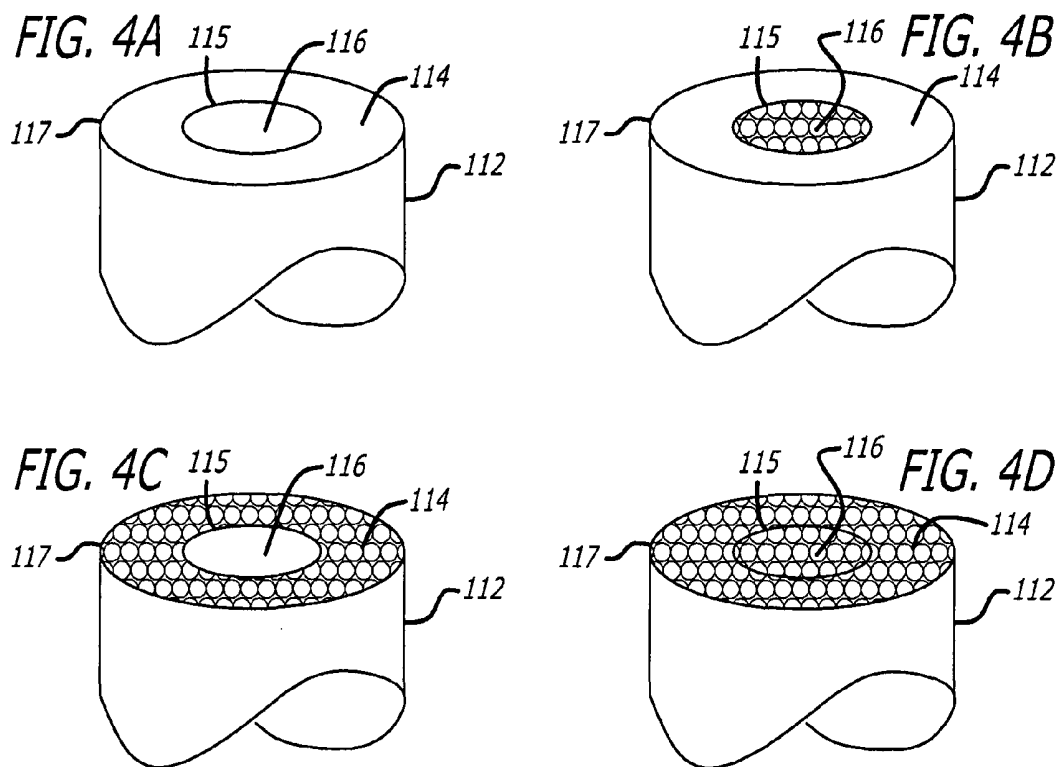


FIG. 3



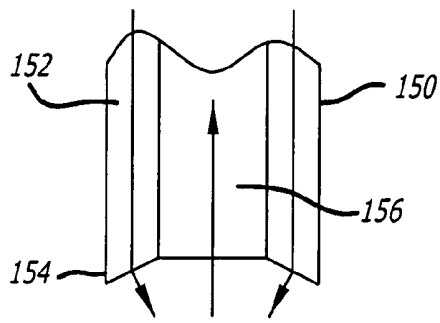


FIG. 6

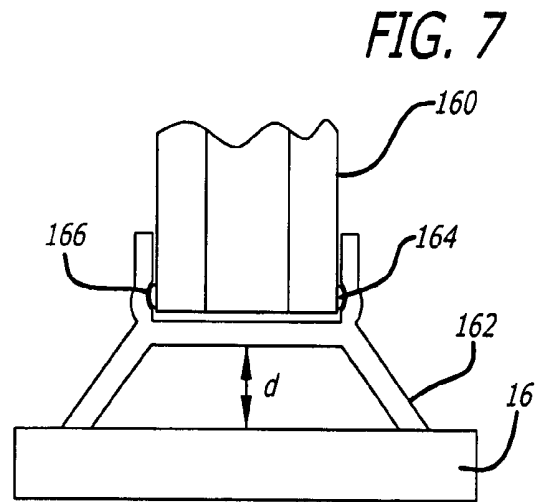


FIG. 7

FIG. 8

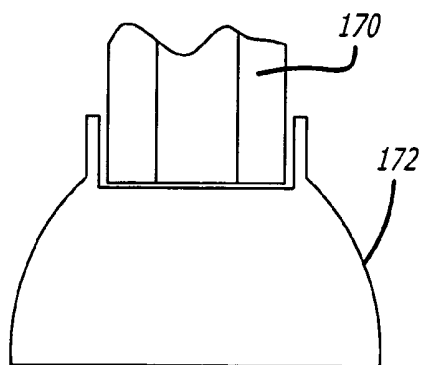


FIG. 9

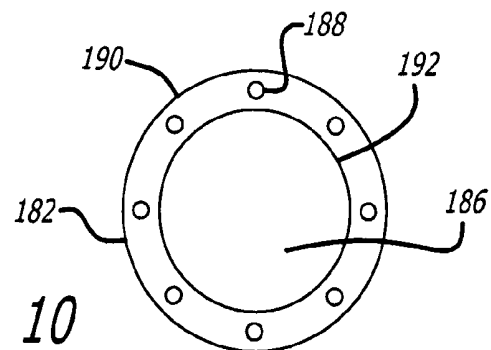
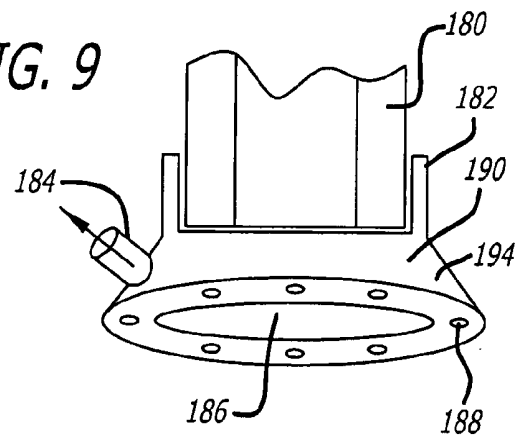
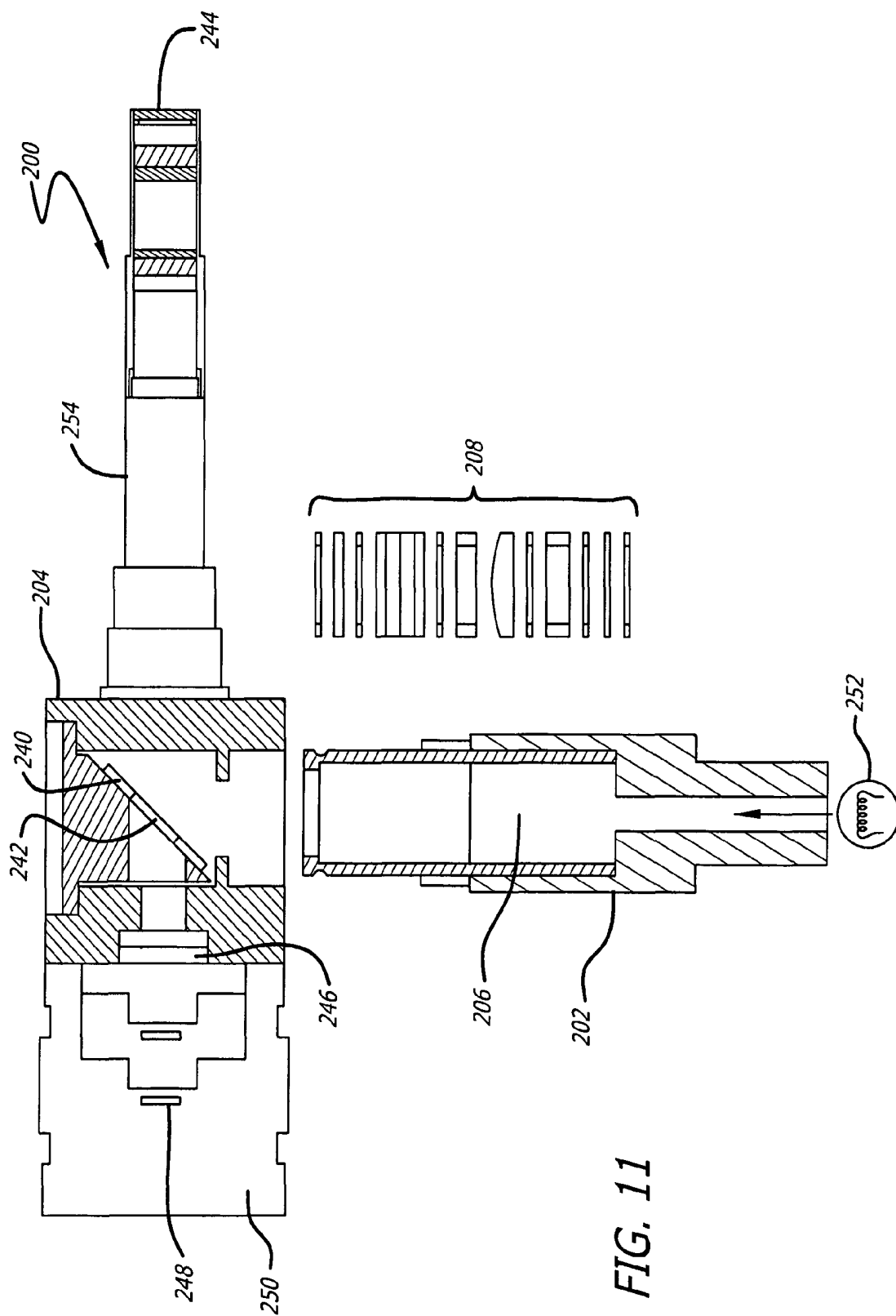
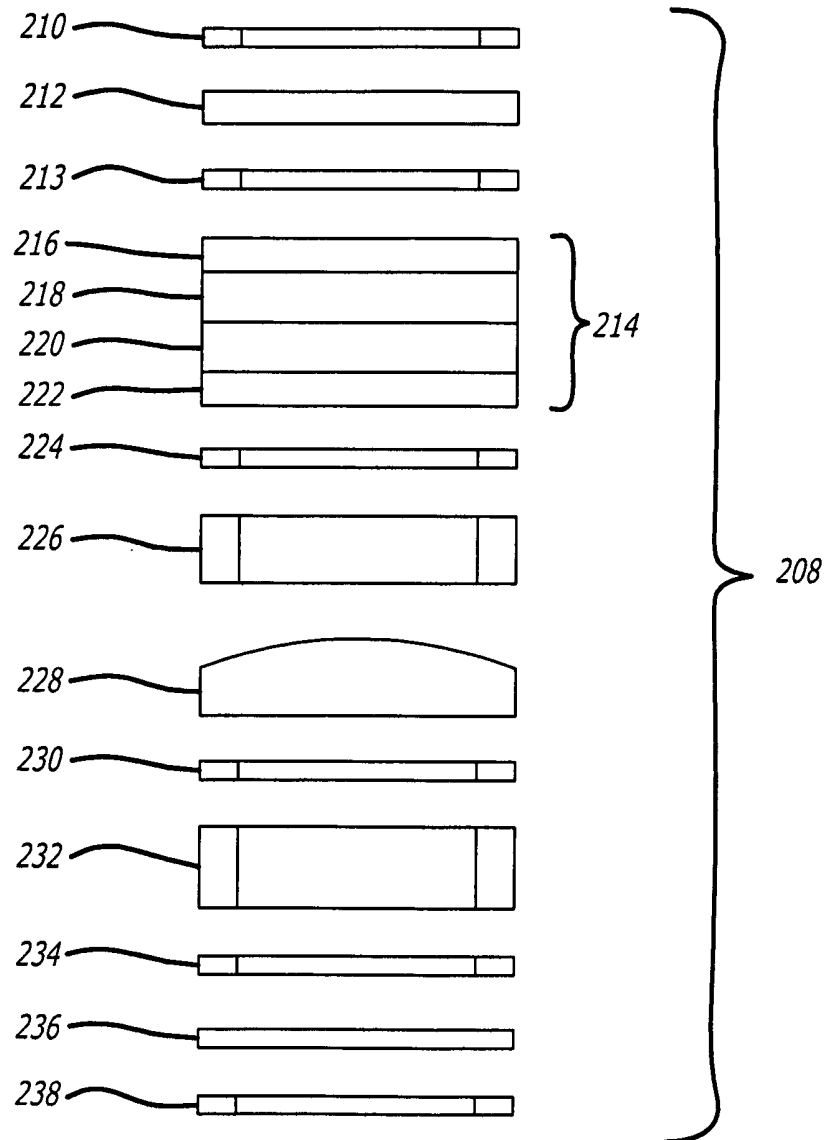


FIG. 10



*FIG. 12*

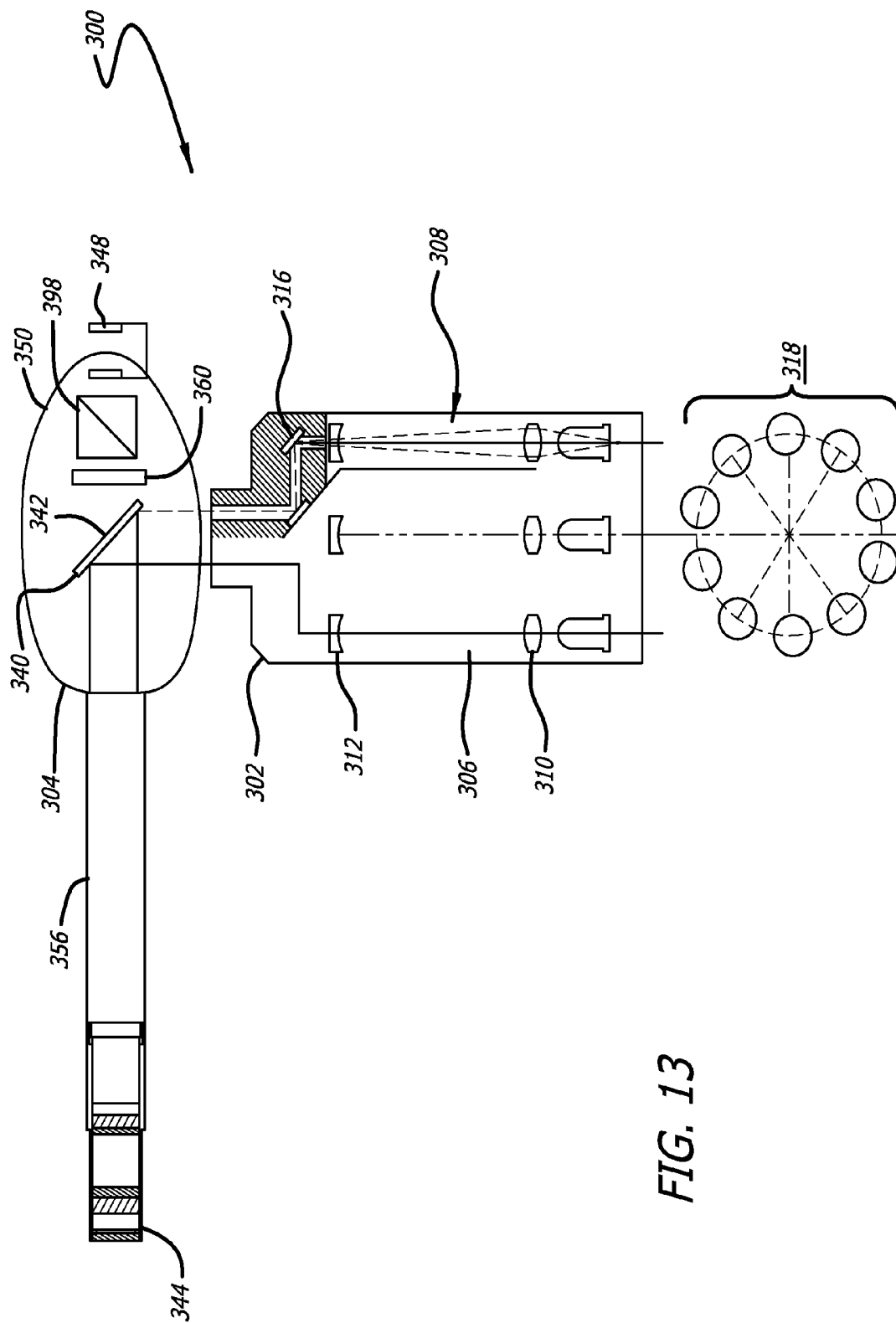
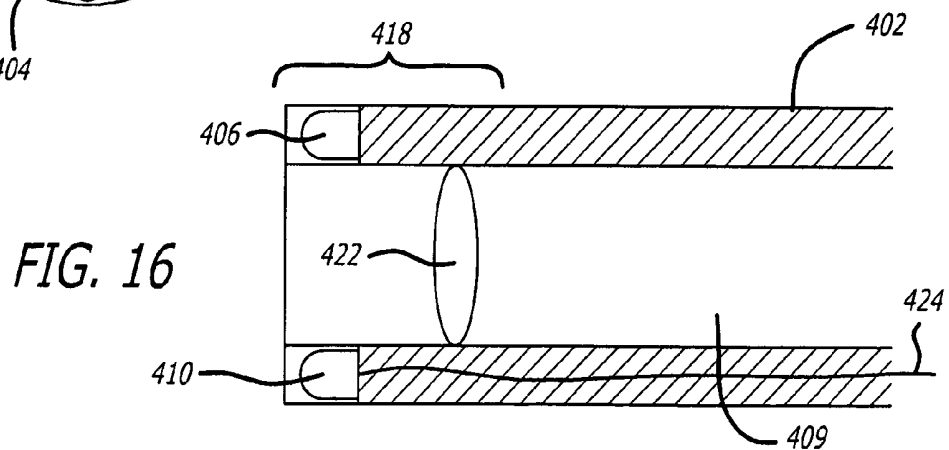
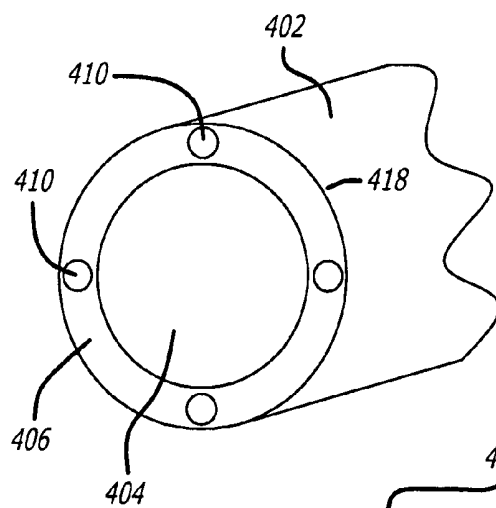
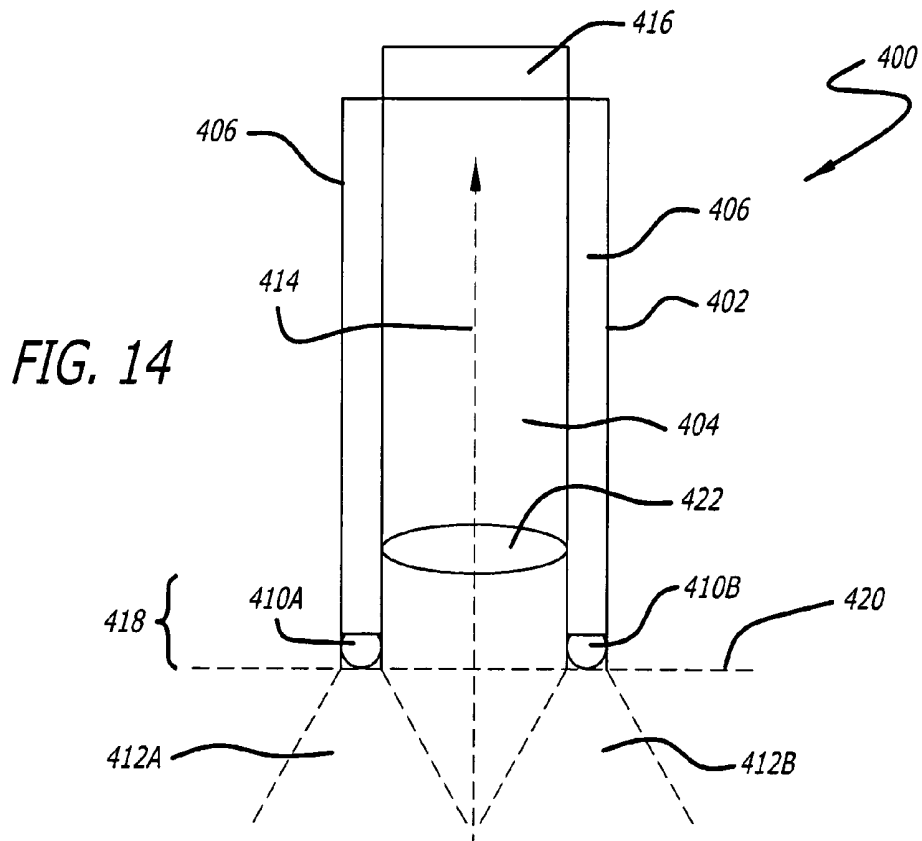
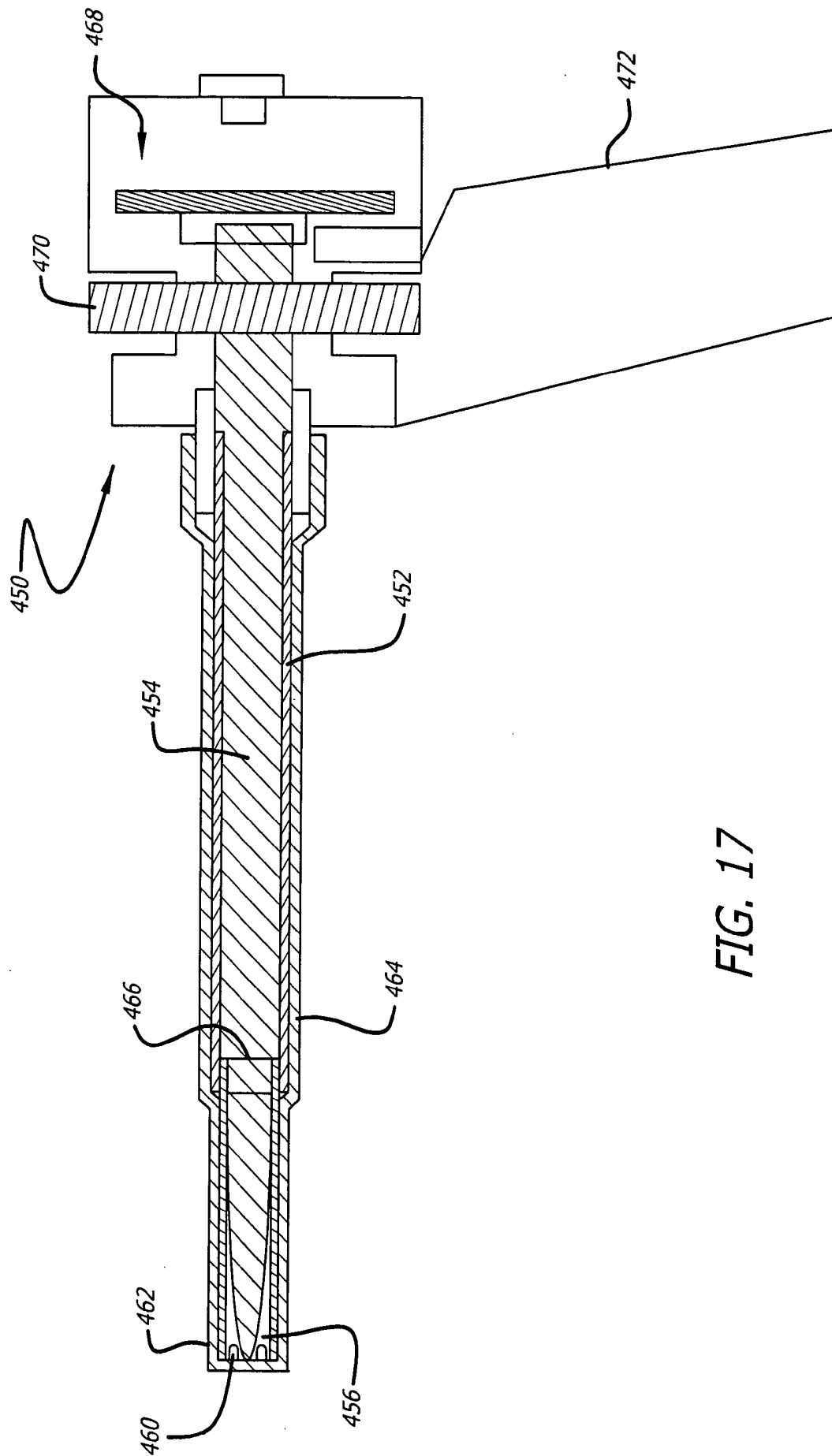


FIG. 13





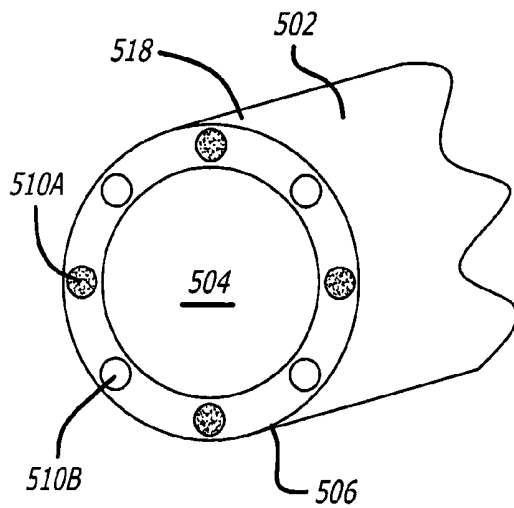
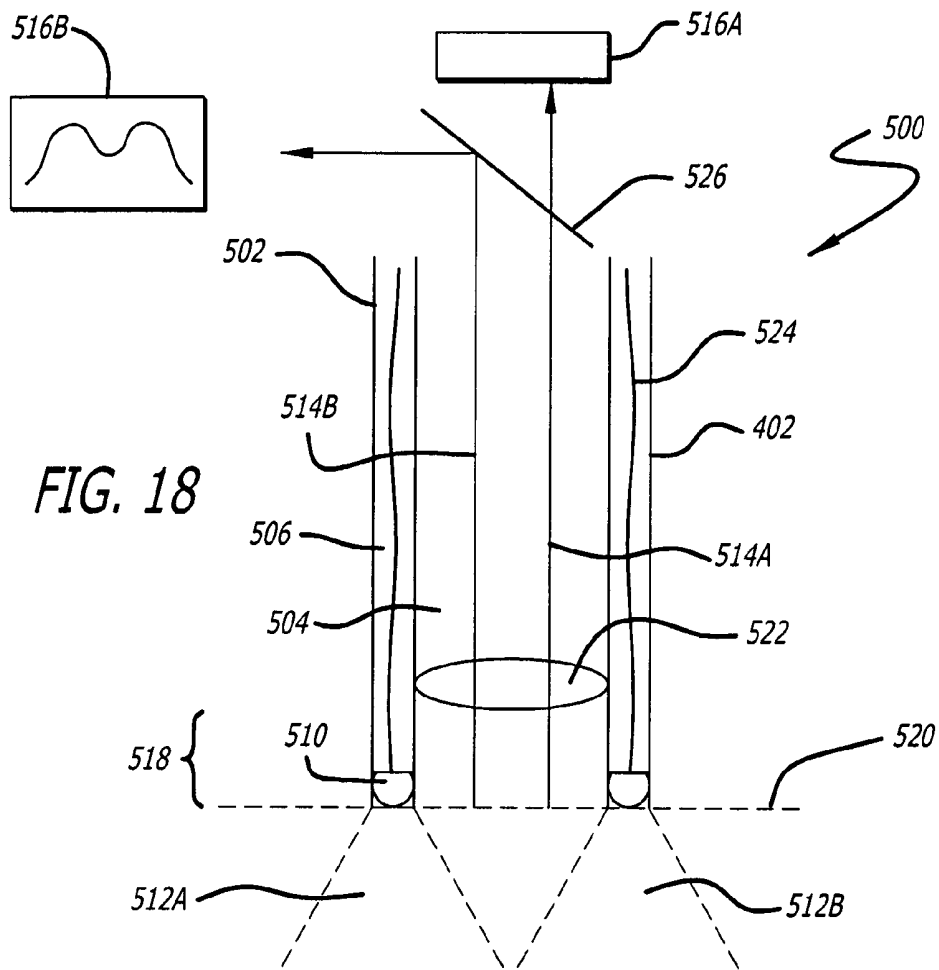


FIG. 20

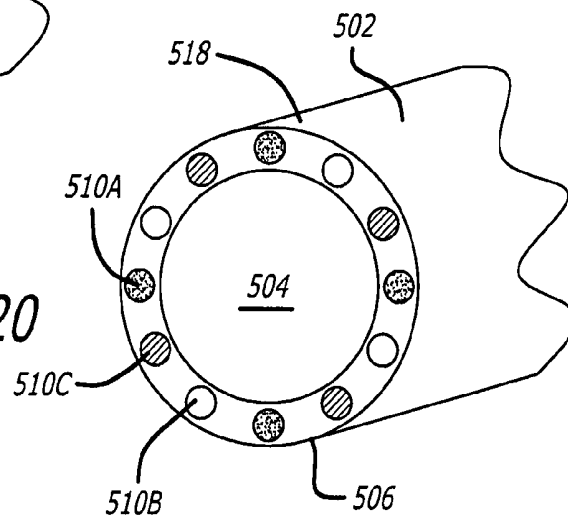


FIG. 21

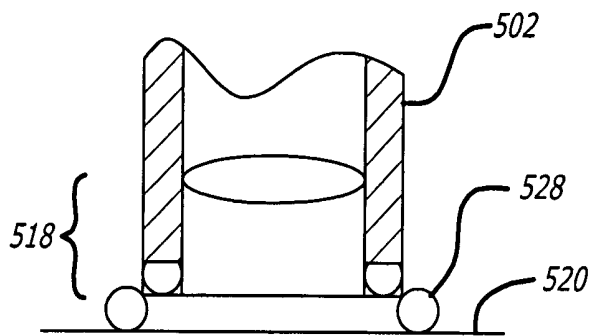
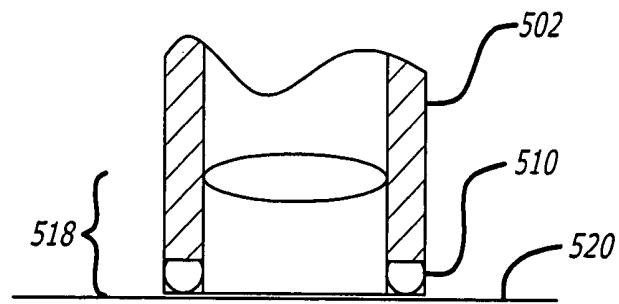
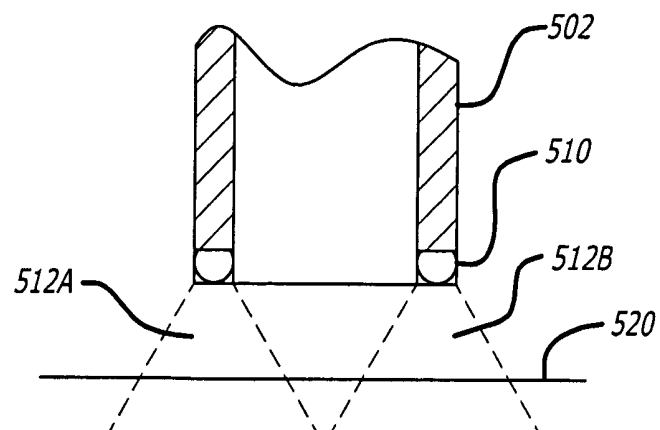


FIG. 22

FIG. 23



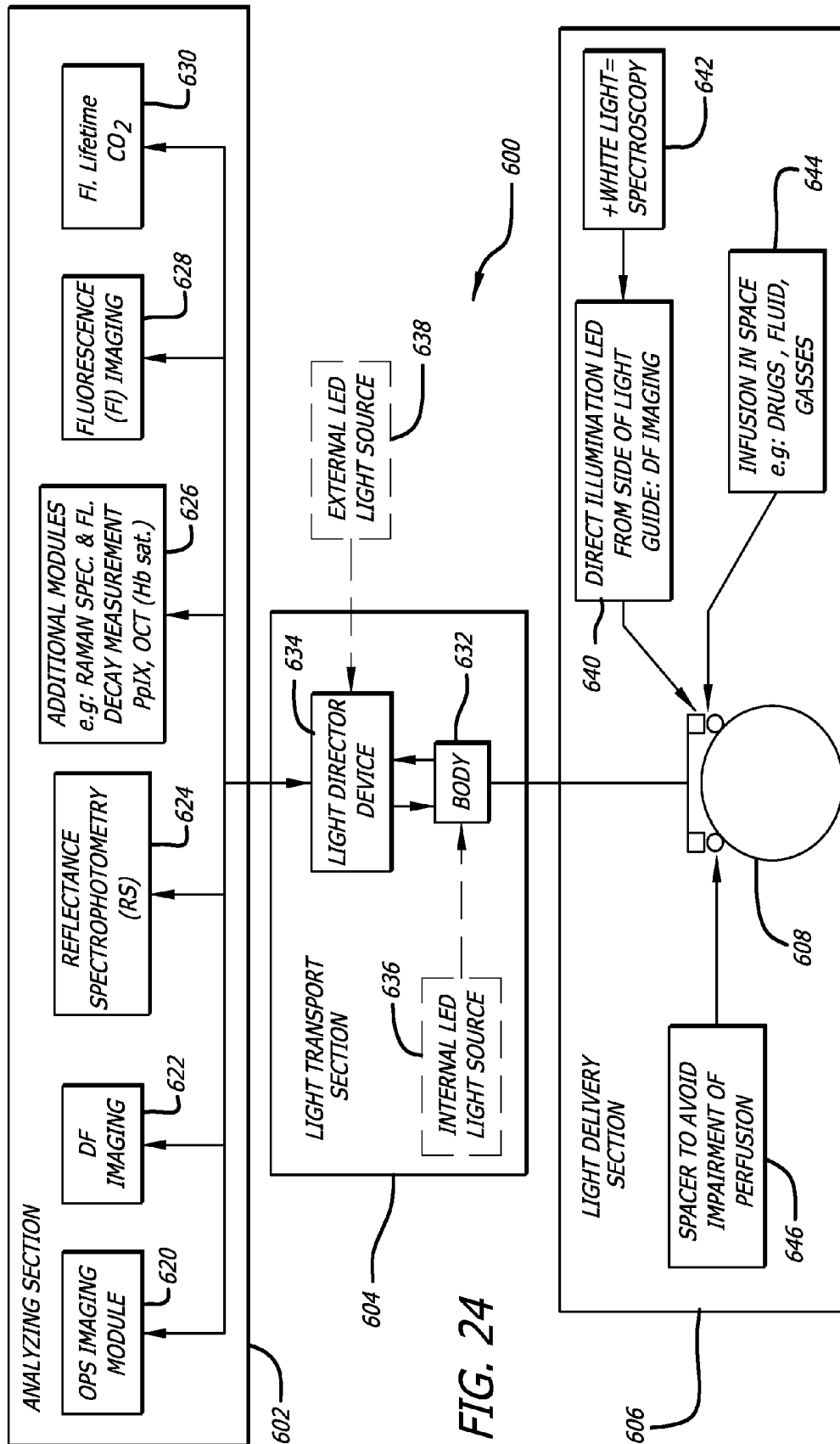
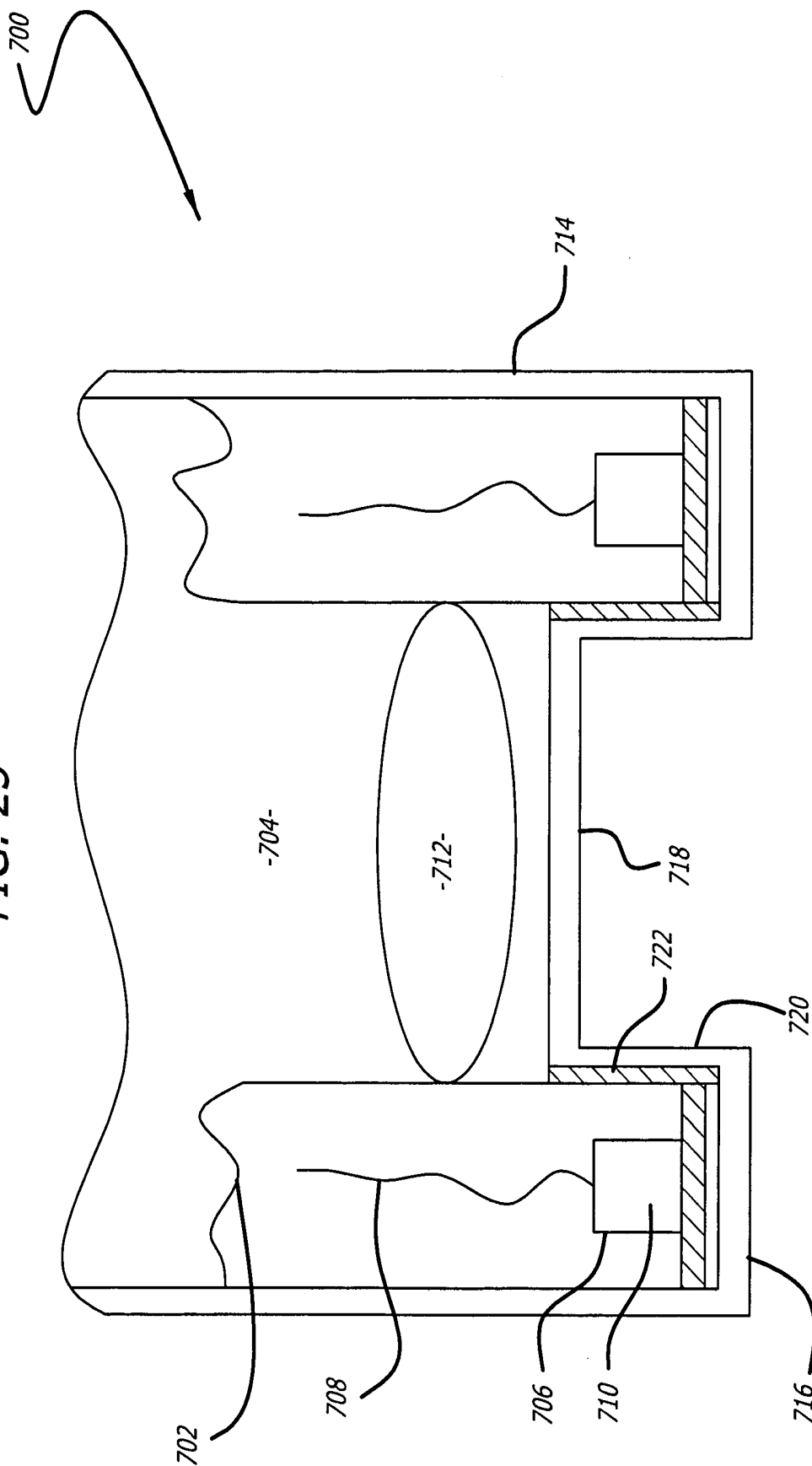
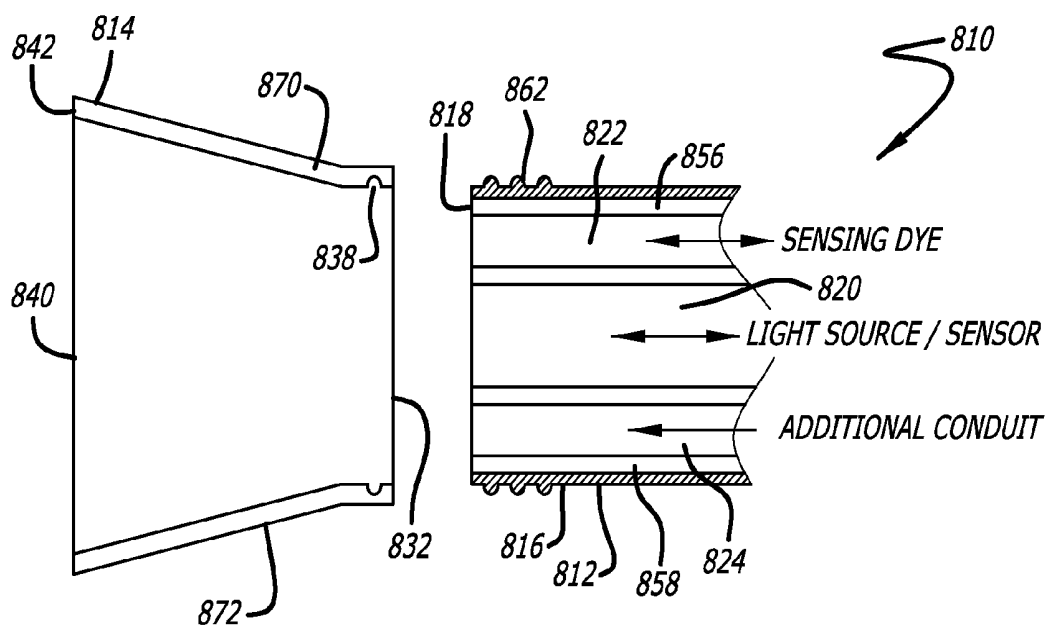
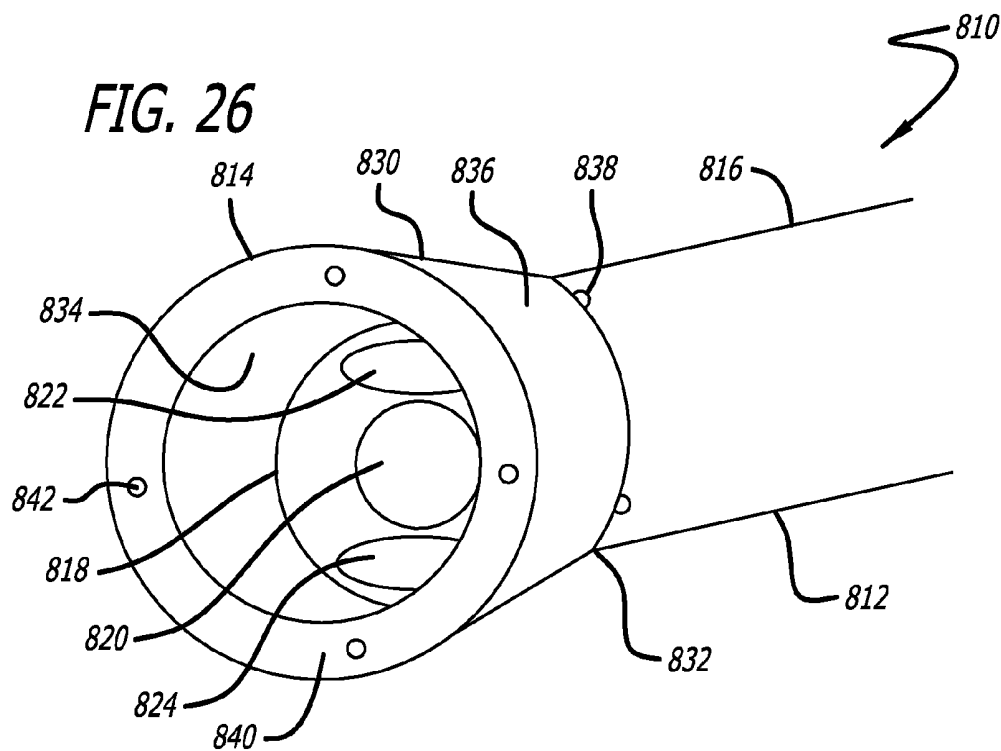
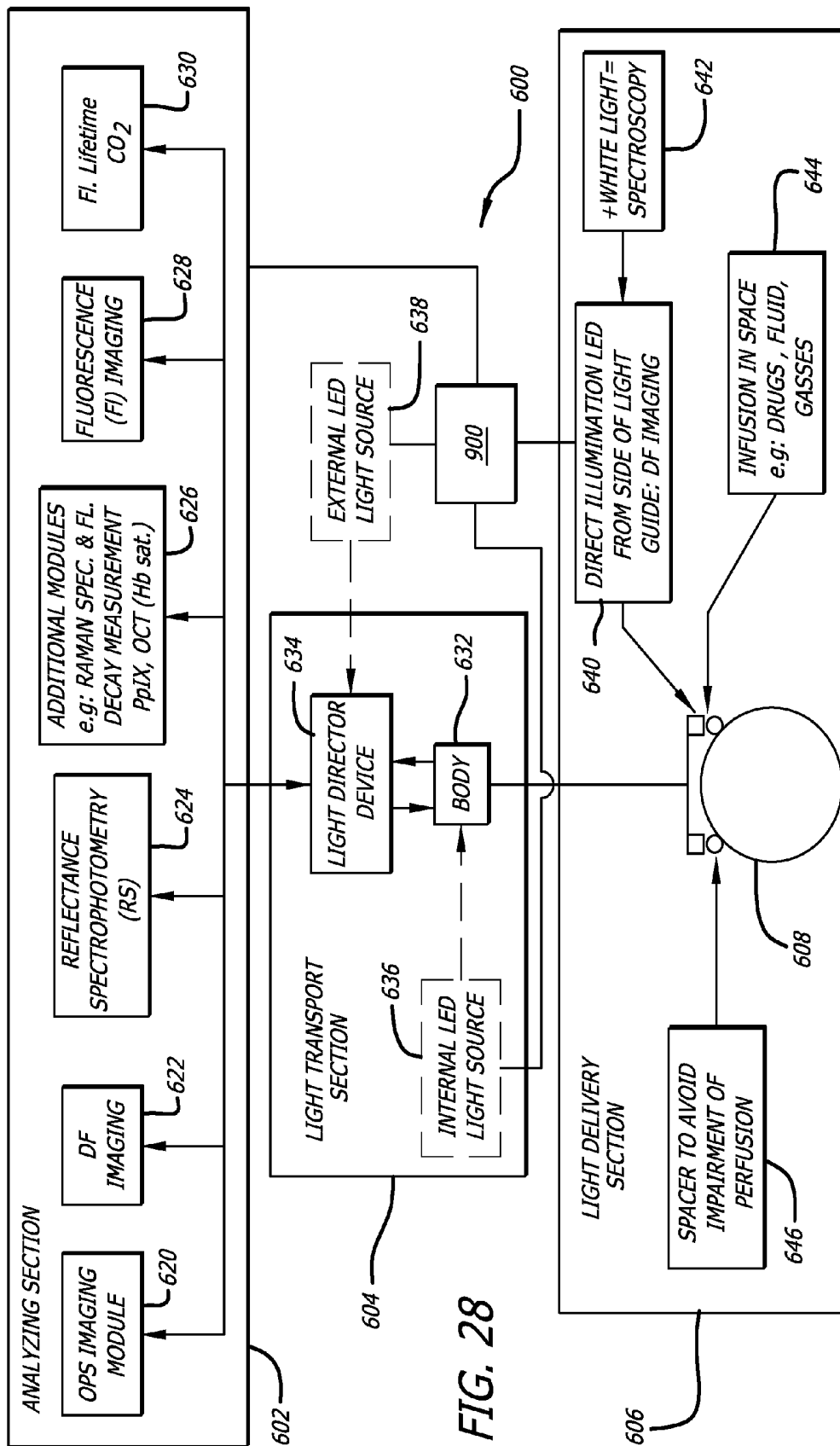


FIG. 25



**FIG. 27**



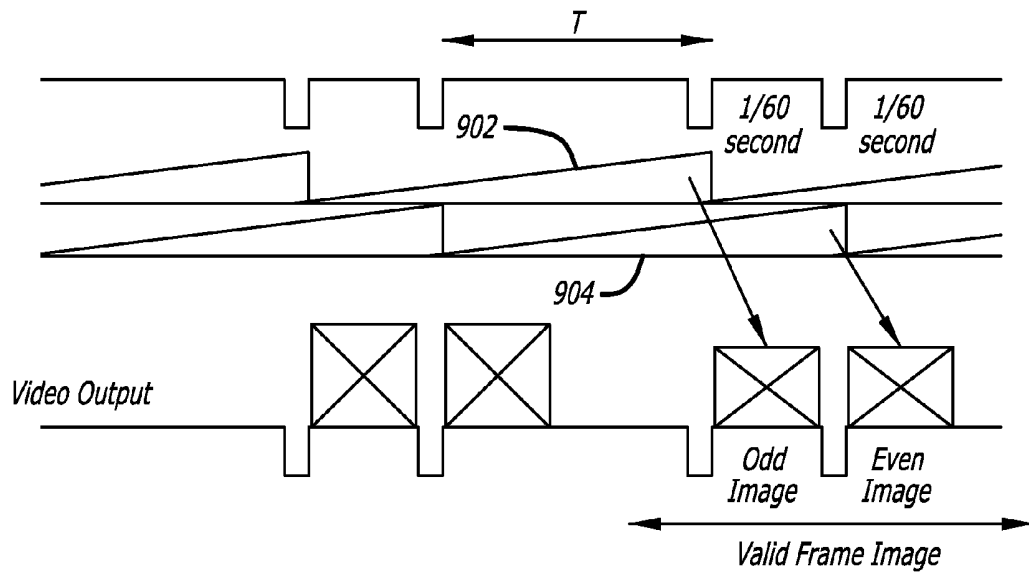


FIG. 29

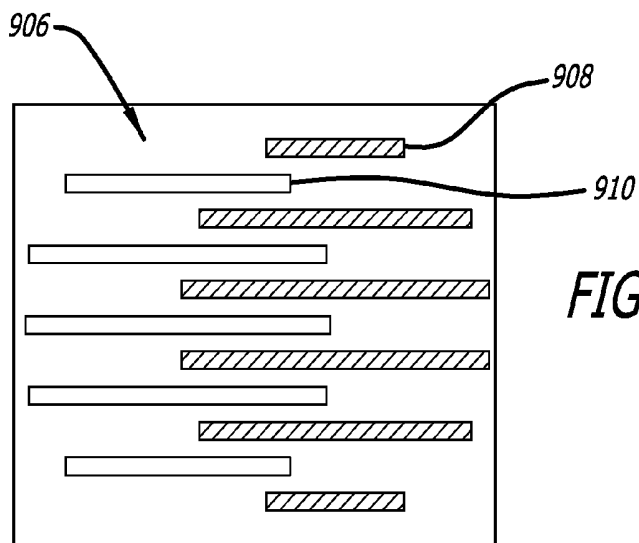


FIG. 30

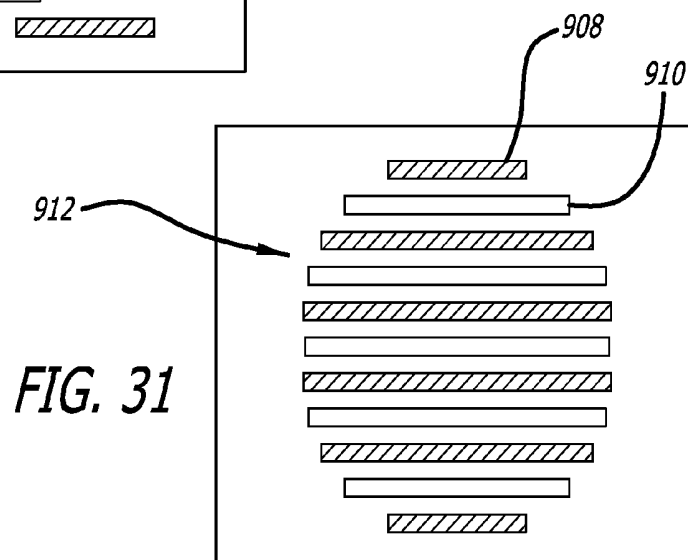


FIG. 31

PULSED LIGHTING IMAGING SYSTEMS AND METHODS

CROSS REFERENCE TO RELATED APPLICATIONS

This application claims priority under 35 U.S.C. section 119(e) from U.S. Provisional Patent Application Ser. No. 60/632,348, entitled "Pulsed Lighting Low Reflectance Imaging Systems and Methods", filed Nov. 30, 2004, by C. Ince, which is also hereby incorporated by reference in its entirety.

BACKGROUND

Currently, physicians typically monitor a number of systemic (e.g. the macrocirculation) hemodynamic parameters when diagnosing and monitoring of the hemodynamic condition of patients. For example, blood flow and pressure are regularly monitored. In addition, a blood sample may be withdrawn from the patient to determine the oxygenation of the red blood cells as well as the oxygen carrying capacity of the circulating blood. Furthermore, a biopsy may be required to determine the functional state of tissue cells (e.g. the oxygenation and viability of tissue cells) of the organ system.

While monitoring these macrohemodynamic parameters has proven successful in diagnosing and monitoring a number of conditions, several shortcomings have been identified. For example, examining macrocirculatory parameters provides little or no information relative to the microcirculatory (i.e. hemodynamics and structure of blood vessels smaller than 250 microns) characteristics of patients. Current research has shown that distress at the microcirculatory level involved in a large number of disease states is not discoverable by monitoring macrocirculation. As such, diseases or other complications evident through microcirculatory monitoring may go undetected and untreated.

It is believed, for example, that improved clinical observation of the microcirculation of human organs would be extremely useful in assessing states of shock such as septic, hypovolemic, cardiogenic and obstructive shock in patients and in guiding resuscitation therapies aimed at correcting this condition. In particular, it has been found that the active recruitment of the microcirculation may be an important component of resuscitation. Additionally, improved clinical observation of the microcirculation would be helpful in observing gross circulatory abnormalities in pathologies such as tumors and cardiovascular disease.

To fully monitor the function of the microcirculation, that is the structure and perfusion of vessels smaller than 250 micrometers, in addition to measuring blood flow it is important to measure and assess whether the blood cells are successful in transporting their oxygen to the microcirculation and thereafter to the surrounding tissue cells. Of particular importance is the assessment of the perfusion of the capillaries, which are between approximately 5 to 10 micrometers, because it is at this level that oxygen is transported by the red blood cells to the tissue cells of the organ for the purposes of respiration and survival. Monitoring the functional state of the microcirculation can thus be regarded as monitoring the ultimate efficacy and function of the cardiovascular system to deliver adequate amounts of oxygen to the organ cells.

It is believed, for example, that improved and comprehensive imaging of the properties of the microcirculation would be helpful in observing and assessing the beneficial effects of therapy during the resuscitation of shock patients. An accurate assessment of both blood flow and oxygen availability at

the level of the microcirculation could thus provide a clinical tool with which to guide resuscitation. A comprehensive way to monitor the microcirculation could generally provide an improved clinical diagnostic tool for evaluating and monitoring the functional state of the microcirculation in the peri-operative phase of treatment.

To date, there have been limits to a comprehensive monitoring of the microcirculation in order to provide the benefits discussed above. Specifically, several factors have limited the ability to evaluate the oxygen transport variables of the microcirculation comprehensively. For example, devices which contact the surface of the microcirculation inhibit their ability to obtain quantitative information about blood flow in the various categories of micro-vessels in the microcirculation by impeding flow due to exerted pressure. Furthermore, current devices and techniques for imaging the microcirculation do not provide the additional needed information about the oxygen availability in the microcirculation or about the adequacy of oxygenation of the tissue cells. This information would be very helpful in assessing the functional state of the microcirculation, specifically its function in allowing adequate transport of oxygen to the tissue cells. Thus, there is a need for an improved system and method for a more effective and a more comprehensive clinical observation of the microcirculation which includes these parameters.

SUMMARY

Some embodiments of an imaging system for analyzing a biological substrate include a light source and a light transport body configured to project light from the light source to the biological substrate and transmit light reflected by the biological substrate. An analysis section is in optical communication with the light transport body and has a video imaging system that utilizes a plurality of sets of field lines integrated over staggered time intervals that overlap in an overlap period. A controller is in communication with the light source and video imaging system and is configured to activate the light source substantially within the overlap period of the video imaging system. In some embodiments of this system, the analyzing section further includes a reflectance avoidance imaging module, a reflectance spectrophotometry module, an fluorescence imaging module and a beam director in optical communication with the light transport body configured to direct at least a portion of the light to at least one of the reflectance avoidance imaging module, the reflectance spectrophotometry module, and the fluorescence imaging module.

Some embodiments of imaging systems for analyzing a biological substrate include an LED light source and a light transport body configured to project light from the LED light source to the biological substrate from the side and transmit light reflected by the examination substrate. An analysis section is in optical communication with the light transport body, is configured to receive light reflected by the biological substrate and has a reflectance avoidance imaging module, a reflectance spectrophotometry module, a fluorescence imaging module and a video imaging system that utilizes a plurality of sets of field lines integrated over staggered time intervals that overlap in an overlap period. A controller is in communication with the LED light source and video imaging system and is configured to synchronously pulse the LED light source substantially within the overlap period of the video imaging system.

Some embodiments of a method of monitoring a patient include providing an imaging system having a light source, a light transport body configured to project light from the light

source to an examination substrate and transmit light reflected by the examination substrate, an analysis section in optical communication with the light transport body and having a video imaging system that utilizes a plurality of sets of field lines integrated over staggered time intervals that overlap in an overlap period and a controller configured to activate the light source substantially within the overlap period of the video imaging system. After providing the imaging system, a biological substrate of the patient is illuminated with pulsed synchronized light from the light source during an overlap period of the video imaging system. Light from below a surface of the biological substrate is received and an image of the biological substrate is generated with the sets of field lines integrated during the overlap period.

Other objects, features, and advantages of the imaging system and method embodiments disclosed herein will become apparent from a consideration of the following detailed description.

BRIEF DESCRIPTION OF THE DRAWINGS

FIG. 1 shows a block diagram of an embodiment of an imaging system for analyzing light reflected from an examination substrate;

FIG. 2 shows a block diagram of an embodiment of an analyzing section of an imaging system;

FIG. 3 shows a schematic diagram of an embodiment of a light transport section configured to project light on and receive reflected light from an examination substrate;

FIG. 4A shows a perspective view of an embodiment of a light transport body of a light transport section;

FIG. 4B shows a perspective view of an alternate embodiment of a light transport body of a light transport section;

FIG. 4C shows a perspective view of another embodiment of a light transport body of a light transport section;

FIG. 4D shows a perspective view of still another embodiment of a light transport body of a light transport section;

FIG. 5 shows a schematic diagram of another embodiment of a light transport section configured to project light on and receive reflected light from an examination substrate;

FIG. 6 shows a side view of an alternate embodiment of a light transport body of a light transport section;

FIG. 7 shows side view of an embodiment of a spacer device coupled to an embodiment of a light transport body;

FIG. 8 shows a side view of another embodiment of a spacer device coupled to an embodiment of a light transport body;

FIG. 9 shows a side view of an embodiment of a spacer device configured to couple to an examination substrate coupled to an embodiment of a light transport body;

FIG. 10 shows a bottom view of an embodiment of the spacer device shown in FIG. 9;

FIG. 11 shows a cross sectional view of an embodiment of an imaging system for analyzing reflected light;

FIG. 12 shows a side view of an optical system for use in the an imaging system for analyzing reflected light shown in FIG. 10;

FIG. 13 shows a cross sectional view of an embodiment of an imaging system for analyzing reflected light having an internal light source positioned therein;

FIG. 14 shows a side cross-sectional view of an embodiment of an imaging system configured to permit side stream dark field imaging of an area;

FIG. 15 shows a perspective view of the distal portion of an embodiment of the imaging system shown in FIG. 14;

FIG. 16 shows a cross sectional view of an embodiment of an imaging system having one or more illumination sources located within illumination passages formed in a body;

FIG. 17 shows a cross sectional view of an embodiment of an imaging system having a body coupled to handle portion;

FIG. 18 shows a schematic diagram of an embodiment of an imaging system for projecting light to a substrate and collecting light therefrom for analysis;

FIG. 19 shows a perspective view of the distal portion of the imaging system shown in FIG. 18;

FIG. 20 shows a perspective view of the distal portion of another embodiment of imaging system shown in FIG. 18;

FIG. 21 shows a side cross sectional view of an embodiment of an imaging system wherein the distal portion thereof is in contact with an examination substrate;

FIG. 22 shows a side cross sectional view of an embodiment of an imaging system wherein the distal portion includes an engaging device thereon;

FIG. 23 shows a side cross sectional view of an embodiment of an imaging system wherein the distal portion is not in contact with the examination substrate;

FIG. 24 shows a block diagram of diagram of an embodiment of an imaging system for imaging microcirculation within a structure and analyzing light reflected from an examination substrate;

FIG. 25 shows a cross sectional view of an embodiment of a cap device which may be affixed to a body of an imaging system;

FIG. 26 shows a perspective view of embodiment of an imaging system configured for sub-surface imaging of an area; and

FIG. 27 shows a side cross sectional view of the imaging system shown in FIG. 26.

FIG. 28 shows a block diagram of diagram of an embodiment of an imaging system having pulsed lighting for imaging microcirculation within a structure and analyzing light reflected from an examination substrate;

FIG. 29 illustrates a diagrammatic view of a video capture sequence in an interlaced frame integration system.

FIG. 30 illustrates a diagrammatic view of a video image of a substantially round object taken with a typical video system using frame integration where the object is moving across the field and the output image is blurred as a result of the movement.

FIG. 31 illustrates a diagrammatic view of a video image taken with synchronized pulse lighting of a substantially round object moving across the field and the output image is not blurred as a result of the movement.

DETAILED DESCRIPTION

Embodiments of the systems and methods disclosed herein provide comprehensive information about the microcirculation by providing multiple modes of optical spectroscopy and imaging in a manner which does not influence the microcirculation. In one aspect, the system avoids reflection of light from the tissue in the various imaging modes. This reflectance avoidance can be provided by reflectance filtering, such as orthogonal polarization or cross-polarization of light or dark field imaging, or by sidestream dark field imaging, wherein, for example, incident and reflected light may not travel down the same pathway.

In order to image flowing cells in the microcirculation, light has to be illuminated on to the surface of the organs, which is the substrate, and a magnifying lens may be used. Use of a specific wavelength of light (e.g. green light) may allow for better observation of the contrasting red blood cells

due to the absorption characteristics of the hemoglobin (hereinafter Hb) in the red blood cells. However, surface reflections from the substrate can interfere with the ability to clearly visualize the underlying microcirculation structures and the flowing blood cells therein. Filtering out of these surface reflection by various methods allows visualization of the blood flow in the underlying microcirculation on organ surfaces by measurement of the images of the moving cells. Reflectance filtering can be achieved by a number of techniques which are known to those of skill in the art. The system and method disclosed herein may utilize some of these known techniques, but some novel ones are disclosed as well.

In some embodiments, the system and method utilizes reflectance avoidance by known techniques of reflectance filtering, such as: 1) OPS imaging, whereby illuminating light and reflected light travel down the same light guide; or 2) Mainstream Dark Field imaging, whereby illuminating light and reflected travel down the same light guide but peripheral illumination is achieved by directing the light through, for example, a hole in a 45° mirror or design of a lens in the illuminating pathway, which impedes transmission of the light through the middle, and/or a lens which poorly allows transmission of the light through the centre is put in the pathway of the light to achieve the same effect.

In other embodiments, a novel method of reflectance avoidance is disclosed which is an alternative to reflectance filtering. This novel approach, referred to herein as Sidestream Dark Field imaging (hereinafter SDF), utilizes external direct light on the tip of the light guide to achieve reflectance avoidance whereby incident and reflected light do not travel down the same pathway. This form of imaging can be provided in combination with a hand-held microscope. A feature of SDF imaging is that illuminated light and reflected light travel via independent pathways. With this modality, the illumination can be placed directly on the tissue and the observations can be made adjacent to it without light crossing over between two paths. The illuminating light source is typically placed on or near contact with the tissue. The scattering of the reflected light is thus outside of the image as most light cross over is below the tissue surface. To date, Mainstream Dark Field imaging has been described as a way of improving contrast and lowering surface reflectance, but it typically utilizes illumination and reflectance light paths that travel up and back the same pathway. In the past, SDF illumination has been applied by ring illumination to improve epi-illumination. It is believed, however, that it has not been applied to achieve true dark field illumination by illuminating one segment of a substrate and observing in another segment images of the microcirculation and its flowing cells. It is believed that SDF imaging has characteristics which make it superior to other modes of imaging.

The foregoing reflectance avoidance imaging systems, whether they utilize OPS, Mainstream Dark Field illumination, or SDF illumination, can be used to enable the comprehensive evaluation of the functional state of the microcirculation. This is achieved by an analysis of the moving cells in the images, which permits the quantitative measurement of red blood cell flow in the capillaries, as well as in the larger vessels of the microcirculation. This measurement is believed to represent a truly sensitive measurement which is indicative of cardiovascular disease and dysfunction. Laser Doppler measurements, for example, provide an over all flux of moving particles in an unidentified compartment of the circulation, but do not have the specificity for measurement of cellular perfusion of these smallest capillaries.

The system and method disclosed herein, in providing reflectance avoidance in combination with optical magnifica-

tion, provides a superior method of measurement of the functional state (e.g. perfusion/oxygenation) of the microcirculation. Next to the measurement of perfusion, morphological characteristics of the microcirculation, such as functional capillary density and micro-vessel morphology, can be measured using reflectance avoidance imaging. Homogeneous perfusion of the capillaries is a prerequisite for normal function of the microcirculation and abnormal perfusion or diminished capillary perfusion is considered an early and sensitive indicator of cardiovascular disease and failure.

The present application thus relates to a variety of imaging systems for analyzing the reflectance of an examination substrate. While the imaging system disclosed herein may be used to analyze the reflectance characteristics of a variety of substrates, it is particularly well suited for non-invasively imaging the micro-circulation with a tissue sample.

In one embodiment, the present application discloses a system for imaging the reflectance of a substrate and includes a light source, a light transport body configured to project light from the light source to an examination substrate and transmit light reflected and scattered by the examination substrate, an analysis section in optical communication with the light transport body and having an orthogonal polarization spectral imaging module or any other of the reflectance avoidance imaging systems, and at least one of a reflectance spectrophotometry module and a fluorescence imaging module.

In an alternate embodiment, the present application discloses an orthogonal polarization imaging system and includes a light source configured to emit white light, a first polarizer to polarize the white light, a light transport body to transport the polarized light to an examination substrate and reflect light from an examination substrate, a second polarizer to filter the light reflected and scattered by the examination substrate, a filter bank containing at least one wavelength filter to filter the reflected light, and an image capture device in optical communication with the light transport body and configured to image the reflected light.

In still yet another embodiment, the present application discloses a method of imaging the reflectance of a substrate and includes illuminating an examination substrate with light, transmitting a portion of light reflected by the examination substrate to a reflectance spectrophotometer, determining a concentration of hemoglobin within the examination substrate based on a spectral characteristic of the examination substrate with the reflectance spectrophotometer, transmitting a portion of the light reflected by the examination substrate to an orthogonal polarization spectral imaging module, and measuring a flow through a vessel within the examination substrate with an orthogonal polarization spectral imaging module.

In one embodiment, the present application discloses a novel manner of applying dark field imaging on the tip of a light guide to provide clear images of the microcirculation on human organ surfaces. This can be accomplished by putting light emitting diodes (LED's) around the tip of the light guide in combination with a separator so that the illuminating light does not enter the reflection light guide directly by surface reflection, but via the internal structures inside the substrate. This modality of reflectance avoidance is a form of dark field imaging which we have called Sidestream Dark Field or SDF imaging and provides remarkably clear images of the microcirculation.

In some embodiments, reflectance avoidance imaging is used to obtain a microcirculatory perfusion index as well as a heterogeneity of flow index in a device that does not impact flow patterns. This may be accomplished by using non-contact modes such as, for example, using a long focal length,

immobilizing the device and substrate by suction at the tip, or utilizing a spacer between the tissue and the light emitting tip.

In one such embodiment, a novel, "castle" type of spacer is utilized to provide distance from the examining substrate and to avoid pressure of the tip on the substrate. In another embodiment, a needle camera is utilized with a spacer to provide a dark field illumination device. In yet another embodiment, a suction device is used with reflectance avoidance imaging techniques.

In another embodiment, a distance spacer is used to achieve reliable capillary perfusion measurements whereby the tip of the image guide does not impede flow in the microcirculation by pressure. In yet another embodiment, reflectance avoidance imaging is used in combination with a space through which fluid, drugs or gasses can be perfused.

In one embodiment, a disposable tip attaches to the end of the device and is removed by a release mechanism so that it can be disposed of without having to touch the disposable.

The utilization of reflectance avoidance in the present invention provides an improved method of observing microcirculatory hemodynamics and functional morphology. Image analysis can provide a plurality of clinical parameters which will have utility for various clinical conditions. The method and device will assist in providing a perfusion index such as a measure of functional capillary density, which is the number of perfused micro-vessels showing per field observed. Other parameters include the distribution and heterogeneity of micro-vascular flow, torsion and functional morphology of the blood vessels, the distribution of diameters of blood vessels, white blood cell kinetics, abnormal red blood cell kinetics (e.g. the presence of micro-vascular coagulation, sludging or adhesion).

For a comprehensive assessment of the functional state of the microcirculation, it may be preferable to have more than just perfusion information. It would also be useful to have information about the amount of oxygen bound to the Hb, which can be provided by reflectance spectrophotometry, and information as to whether the tissue cells are getting sufficient amount of oxygen, which can be provided by measuring tissue CO₂ by sensing the CO₂ in the inside of the disposable, using, for example, CO₂ sensitive fluorescence quenching dyes. The light guide can then be used to excite the dye with a pulse of light and a detector which measures the CO₂ dependent quenching of fluorescence life time would provide the measurement. Also, mitochondrial energy states by NADH via fluorescence imaging can be obtained. Information may be obtained about whether there is movement of the red blood cells in the microcirculation, whether the red blood cells are transporting oxygen (i.e. Hb saturation), and whether the tissue cells are getting enough oxygen (tissue CO₂ measurement and/or NADH fluorescence imaging).

In some embodiments, reflectance spectrophotometry in conjunction with reflectance avoidance is used to assess the adequacy of oxygen availability. This may provide for the assessment of microcirculatory oxygen transport. In some embodiments this can be accomplished by an analysis of the full reflected spectrum of light (e.g. 400-700 nm). In other embodiments it is accomplished by an analysis of discrete wavelengths outputs of a color sensitive imaging device. Microcirculatory Hb saturation, microcirculatory Hb concentration, and microcirculatory hematocrit can all be measured.

In some embodiments, the SDF imaging technique is combined with the use of different wavelengths LED's wherein the images are normalized and Beer Lambert equations are applied.

In some embodiments, NADH fluorescence imaging is used to measure the adequacy of the need for mitochondrial oxygen. This can be used to assess tissue cell dysoxia.

In some embodiments, fluorescence spectroscopy is used for tissue cell diagnostics using endogenous molecules, reporter genes or external indicator dyes. With appropriate filters, apoptosis can be detected (e.g. via annexin fluorescence), green fluorescent labeled cells used in gene therapy could be located in terms of their efficacy in homing in on the target.

In one embodiment, a method of imaging the microcirculation by avoiding surface reflections is combined with reflectance spectrophotometry, Raman spectroscopy, fluorescence spectroscopy and/or other types of spectroscopic modalities, such as light scatter measurements or optical coherence tomography.

In some embodiments, the device is a light guide based system wherein emission and excitation light travels via light guides. In some embodiments, the images are detected at the tip with a tip camera. The device may have a fused silicon lens which will allow 360 nm to pass in order to enable NADH fluorescence imaging. The device can be either hand held or a flexible endoscopic type.

In addition, to direct contact imaging, the reflectance avoidance imaging system disclosed herein may also be capable of operating in a non-contact mode which makes use of a spacer to avoid pressure in the tissue surface which may impede blood flow therethrough. Various spacer options exist, including;

- a. plastic upside down cup attached as disposable;
- b. a doughnut shaped spacer (which can be inflatable) with an upside down situation/cup;
- c. a device (e.g. a plug for around the scope end), such as a concentric ring with suction ports, for providing suction through little holes around the perimeter of the scope thereby immobilizing the perimeter but leaving the microcirculation in the field of view unstressed; or
- d. a transparent cushion either solid, air inflatable or filled with fluid.

What is also disclosed is a non-contacting tip for endoscopic use. In one embodiment, long focus distance imaging can be used to observe retinal microcirculation. This modality can be used to monitor eye diseases and as a monitoring tool during surgery to monitor brain function non-invasively. In the retinal application imaging light can be pulsed and small clips of moving images used for monitoring, thus minimizing retinal light exposure.

In one embodiment, the system is configured to operate in a no contact mode without use of a spacer. Thus, the system may be used during brain surgery or heart surgery. Any movement of the object surface can be corrected by image processing either on-line or after a delay.

In one embodiment the light guide system has an L-shape at the end. Here a 45° mirror creates the bend and LED illumination, using SDF, imaging is present at the tip, with or without a spacer and/or suction module. This embodiment may be used to inspect the sides of hollow spaces such as is present in the digestive track.

In another embodiment, large objective magnification may be used. For example, image processing software may be used to immobilize or stabilize the images, thereby allowing for better image processing of the movements.

In still another embodiment, magnification of the substrate image can be influenced in several ways. For example, different lenses may be used (different spacer on the tip), or movement of exiting lenses by an opto-mechanical system, or in the electronic mode a larger number of pixel CCD or

CMOS chips, which are known to those of skill in the art, or a larger density of pixels in the chip can be utilized. Movement of the CCD or CMOS can also be used to influence magnification.

In still another embodiment, any number of specified color cameras may be used with the present system. For example, a choice of color or combination of colors would allow images to be generated of the saturation of the Hb of the red blood cells in the microcirculation. A further embodiment involves looking at only the red output of a color camera and to filter out of the rest of the image. This would result in red cells moving in a white background.

Use of a high speed rate (i.e. higher than video rate) can be used for obtaining a proper velocity measurement in conditions in which red blood cells are moving faster than the video rate.

In some embodiments, a CO₂ measurement of the tissue in the field of view can be made simultaneously with a reflectance avoidance flow measurement and an oxygen availability measurement, such as with spectrophotometry, as a measure of tissue wellness.

In one embodiment, a disposable spacer (e.g. upside down cup) may be employed. In this embodiment, a CO₂ sensing dye can be impregnated with which CO₂ can be sensed within the cup environment. The dye works to provide a fluorescence decay measurement and the excitation and emission light of this dye in the disposable tip can be measured through the light guide. The CO₂ measurement can be combined with a reflectance avoidance flow measurement, such as an OPS or SDF imaging based perfusion measurement. Furthermore, a CO₂ probe may be inserted into the nose of a patient to assess tissue pCO₂ and combine this information with simultaneously measured perfusion (e.g. by OPS or SDF imaging) and oxygen availability (spectrophotometry) measured sublingually. In another embodiment, the CO₂ probe may be used rectally. These measurements may be made continuously. The sensor may be embedded within a pliable cushioning material. For example, the sensor may be positioned within a sponge so as to trap and sense the CO₂ sufficiently.

The CO₂ sensor can be used in the nose and/or rectally as alternative locations for a separate sensor which is then integrated in the measurement. This can be in single or in multi mode. The latter technique, which makes use of more than one CO₂ sensor, will give information about regional heterogeneity. Using multi locations is believed to be a new use of a CO₂ measurement.

In some embodiments, a laser can be included as a therapeutic modality. This can be accomplished, for example, by the use of dark field illumination in which the laser goes through the hole in the slanted mirror. In this embodiment, reflectance avoidance imaging is combined with the use of the laser for photodynamic therapy (e.g. for cancer) or to coagulate micro-vessels in port wine stains or other cosmetic corrective procedures.

In another embodiment, reflectance avoidance imaging is used to observe the microstructure of the wound, and temperature is sensed by a solid state or thermo-sensitive color sensor as well as by optical spectroscopy to measure the water content. It is thereby that wound perfusion (via e.g. OPS or SDF imaging), wound temperature and edema (water content) will give a comprehensive measurement of the phase of wound healing and allow assessment of the response to therapy.

In the photodynamic embodiment (where the patient receives a photosensitive drug) it is possible to apply fluorescence in combination with reflectance avoidance for detection of the drug (which accumulates in tumors) or for

enhanced fluorescence in ALA induced protoporphyrin fluorescence. Combining a therapeutic laser in the device would make it possible to deliver photodynamic therapy directly to the area of high fluorescence.

Alternative illumination modalities may include pulsing the LED illumination in combination with synchronization with a camera for the measurement of high blood flow velocities. Another alternative includes the use of an optical foil, acting as a light guide, or other material which may be wrapped around the tip of the probe providing illumination from the side of the tip as an alternative way of illuminating the object and accomplishing reflectance avoidance. This is similar to the method which is accomplished by the use of optical fibers placed around the out side of the scope.

Other embodiments which include laser therapies include the use of reflectance avoidance imaging to verify the effectiveness and allow for the accurate titration of laser doses. A second example is the use of photodynamic therapy for on-line treatment of photosensitized tumors.

In another embodiment, a custom spacer is disclosed in which it is possible to introduce a drug or gas to the field of observation and measure the reactivity of the blood vessels (i.e. losses of which are an indication of poor function). This spacer could be a suction spacer which would provide space in the field of view to ensure that there is no contact with the tip and also provide space to inject a drug (for microcirculatory responsiveness) or for calibration that may be needed for the embodiment which utilizes a CO₂ sensor placed in the probe. Drugs which can be considered challenges to the microcirculation are vasodilators acting on specific locations of the microcirculation e.g. acetyl choline, lidocaine or nitrate. Others include vasopressors, such as noradrenaline or dobutamine. This modality can also be used in local treatment of tumors by application of a topical administration of a chemotherapeutic drug.

Measuring the reactivity of the blood circulation to challenges (also given systemically) via, for example, trend measurements, yield parameters which give additional information than a snap shot analysis. Response to therapy of the microcirculation can be monitored continuously providing on-line information about the functional state of the microcirculation during illness.

A further challenge can be induced through a specialized spacer which applies a momentary suction pulse and measures the time of microcirculatory refill.

In some embodiments multi-wavelength imaging can be used for the measurement and analysis of Hb saturation images. The object is sequentially or simultaneously illuminated by specific colored LED's, placed in SDF mode, which are chosen at specific wavelengths along the absorption spectrum of Hb, such that when combined in a composite image they provide an image of the distribution of Hb saturation (or Hb concentration or Hematocrit) of the cells of the microcirculation. A second embodiment for achieving the same objective utilizes white light. The reflected light is then split by a multi-wavelength optical member which may consist of mirrors and filters which project two or more images each at a different wavelength onto the imaging device to allow reconstituted saturation images to be made.

In one embodiment the use of fluorescence SDF imaging (endogenous leucocyte fluorescence), or observing light scatter, to view differences between cells moving in the circulation (i.e. leucocytes scatter more light than red blood cells) and combining such imaging, with or without filtering of special wavelengths, optical conditions permit the observation and quantification of the amount of leucocytes flowing in the microcirculation. Such a measurement would allow quan-

tification of the immune status of the observed field of view by counting the amount of leucocytes and/or observing the kinetics of cell sticking or rolling.

In one embodiment, annexin fluorescence can be used for the detection of apoptotic cells. A combination of fluorescence techniques includes but is not limited to annexin-labeled cells which will allow for the visualization of apoptotic cells which are directed to programmed cell death, a precursor to necrosis and cell death. These measurements may be important in assessing cell failure in cardiovascular disease, sepsis and in identification and staging of the severity of cancer, or other stages of diseases such as inflammatory bowel disease. In this application fluorescence labeled annexin is administered to the patient, or applied topically to the site of interest and utilizes the fluorescence mode of the scope. In the fluorescence mode of the scope we describe a hand tool (a fluorescence boroscope) such as described for the reflectance avoidance imaging but in which fluorescence modality is utilized. Reflectance avoidance imaging can be used to improve fluorescence imaging, by filtering or avoiding surface reflections, and can be applied in the boroscope application or also in fluorescence endoscopy where, to date, the combination of fluorescence and reflectance avoidance imaging has not been disclosed.

In this embodiment, the appropriate choice of filters can be used to image mitochondrial energy states (NADH levels) through the use of fluorescence. NADH in vivo fluorescence imaging involves dual wavelength fluorescence combined with reflectance avoidance imaging to correct for changes in absorption in the image, which can be caused by variation in Hb (which is an absorber) in the vessels in the image (results in heterogeneous images). In addition, fluorescence spectrophotometry may be combined with reflectance avoidance imaging to allow cell diagnostics during surgery directly at the bedside. Tissue cell diagnostics will target the functional state of the mitochondria by measurement of the energy of the mitochondria by NADH fluorescence, the gold standard for assessment of tissue dysoxia. Such fluorescence imaging can also be used in conjunction with diagnostic dyes for identification of apoptosis or tumor cells and reporter genes during gene therapy. Combination of fluorescence dyes and cell labeling techniques can be used by this modality (with appropriate filters) to observe and quantify the degree of degradation of the glycocalyx lining of the endothelia cells. This observation provides a microcirculatory indication of the severity of cardiovascular disease. Finally measurement of the time course of transport through the microcirculation of a pulse of fluorescent dye allows microcirculatory flow at the capillary level to be quantified when detected by fluorescence.

In some embodiments, reflectance avoidance imaging will be combined with Raman spectroscopy, thereby combining microcirculatory reflectance avoidance imaging with information about the constituents of the tissues.

The above embodiments can be used in an endoscopy mode. For example, dark field endoscopy, OPS imaging, and/or side illumination can be used to make observations in the gastric tract, with for example, the L-tip device discussed above. Polarization can be achieved at the tip of a flexible endoscope. Dark field illumination can be used in the same way by concentric illumination. A light conducting foil can be used at the outside. A 45° mirror can be included at the tip for observation of the sides of the gastric tubes. Thin scopes can be made for pediatrics.

In some embodiments, optical coherence tomography can be used for measurement of optical path-length using Beer Lambert as a quantitative measurement.

Sublingual Near Infra-red Spectroscopy can be used in the transmission mode or in the reflectance mode to measure total oxygenation of the tongue.

The foregoing methodologies for comprehensive imaging of the microcirculation provide a useful clinical tool in assessing states of shock such as septic, hypovolemic, cardiogenic, and obstructive shock in patients and in guiding resuscitation therapies.

FIG. 1 shows a block diagram of an embodiment of a reflectance imaging system. The imaging system 10 includes an analyzing section 12 and a light transport section 14 configured to project light on and/or receive reflected light from an examination substrate 16. In one embodiment the light transport section 14 may include an internal light source 18 therein configured to provide light of at least one selected wavelength and/or polarization to the examination substrate 16. Optionally, the internal light source 18 may be used with or may comprise a source of white or full spectral light thereby enabling spectral analysis of light reflected by the examination substrate 16. In an alternate embodiment, an external light source 20 may be in optical communication with the light transport section 14 and configured to illuminate the examination substrate 16. Optionally, the imaging system 10 may include both an internal light source 18 and an external light source 20. As such, the internal and external light sources may have the same or different wavelengths and/or polarizations. In another embodiment, an ancillary illuminator 22 may be used to illuminate the examination substrate 16. As shown, the ancillary illuminator 22 directly illuminates the examination substrate thereby foregoing the light transport section 14. The various components of the analyzing section 12 and the light transport section 14 will be described in greater detail below.

Referring again to FIG. 1, in one embodiment the analyzing section 12 includes any number of modules configured to analyze light reflected from the examination substrate 16 and transported to the analyzing section 12 by the light transport section 14. In the illustrated embodiment, the analyzing section 12 includes an orthogonal polarization spectral (OPS) imaging module 30, a reflectance spectrophotometry (RFS) module 32, and a fluorescence (FLS) imaging module 34. Any number of additional modules 36 may be included in the analyzing section 12. Exemplary additional modules include, without limitation, Raman spectroscopy modules, optical coherence tomography modules, dark field imaging including side stream dark field imaging (See below), and various light scattering measurement modules.

As shown in FIGS. 1 and 2, the OPS imaging module 30 receives a light sample 40 from a beam director 98. The light sample comprises light reflected from the examination substrate 16 and transmitted to the beam director 98 by the light transport section 14. As such, the OPS imaging module 30 is configured to image the examination substrate 16 using either dark field or non-dark field illumination. Thereafter, the light sample 40 may encounter a polarizing section 42 having one or more optical polarizers therein. The polarizing section 42 permits only light of a selected or desired polarization to transmit therethrough, thereby filtering the light reflected by the examination substrate 16 and improving image quality. In an alternate embodiment, the OPS imaging module 30 may incorporate a variety of other optical devices or methodologies to optimize image quality. The polarized light 44 is then incident upon a filtering section 46 having one or more optical filters therein. For example, in one embodiment the filtering section 46 contains at least one narrow band pass filter therein configured to permit light within a desired wavelength range to be transmitted therethrough. Exemplary narrow band pass

filters include, without limitation, from about 380 nm to about 450 nm (violet filter), from about 445 nm to about 510 nm (blue filter), from about 495 nm to about 580 nm (green filter), from about 575 nm to about 595 nm (yellow filter), from about 590 nm to about 625 nm (orange filter), from about 615 nm to about 710 nm (red filter), and from about 690 nm to about 910 nm (color or photo infrared filter). Optionally, the OPS imaging section 30 may include filters enabling ultra-violet radiation to transmit therethrough. In an alternate embodiment, the filtering section 46 receives light from the light transport section 14 prior to the light sample 40 being polarized.

Referring again to FIG. 2, the filtered light 48 is then transmitted from the filtering section 46 to an image capture device 50. Exemplary image capture devices 46 include, without limitations, charge coupled devices (CCD) and photomultiplier devices. For example, in one embodiment a CCD chip having about 1000 by 1000 pixel resolution or higher may be used. Optionally, images captured at various wavelengths may be captured and compared to permit image normalization. In an alternate embodiment, an image capture device 50 may be utilized to correct for motion effects and aberrations. The image capture device 50 forms an image of light reflected from the examination substrate 16 and transmitted to the OPS imaging section 30 by the light transport section 14. (See FIG. 1). In the illustrated embodiment, the image capture device 46 is in communication with a processor and display device 52. The processor and display device 52 may be used to process information from the image capture device 50 and display the information in any number of ways. Exemplary processor and display devices include, without limitations, computers and display terminals.

As shown in FIG. 2, the OPS section 30 may include a light modulator 54 and/or an OPS optics suite 56. The light modulator 54 may be used to segment the sample light 40, thereby providing a stroboscopic effect thereto. Exemplary light modulators 54 include, without limitations, light choppers, shutters, and light valves including liquid crystal light valves. An OPS optics suite 56 may be used to focus, defocus, collimate, or otherwise refine the light sample 40 transmitting through the OPS imaging section 30. Exemplary components which may be used within the OPS optics suite 56 include, without limitations, mirrors, positive lenses, negative lenses, acromats, compound lenses, astigmats, windows, flats, adaptive optics, holographical optical elements, spatial filters, pinholes, collimators, stages, and beam splitters. The light modulator 54 and the OPS optics suite 56 may be positioned at various locations within the OPS imaging section 30.

Referring again to FIG. 2, the reflectance spectrophotometry module 32 includes a spectrophotometer 70 coupled to a RFS image processor 72 for computing and displaying spectral characteristics of the light reflected from the examination substrate 16. (See FIG. 1). For example, full spectrum (e.g. white) light is used to illuminate an examination substrate. Thereafter, the light reflected by the examination substrate 16 may be captured and the spectral characteristics thereof may be examined to measure a variety of characteristics of the examination substrate 16, including, without limitation, hemoglobin saturation and hematocrit concentration. Exemplary RFS image processors 72 include, without limitation, CCD and CMOS chips and photo-multiplier devices coupled to processors and display monitors. As such, the spectrophotometer 70 is in optical communication with the light transport section 14. In one embodiment, an RFS optics suite 74 may be used to process and refine the light received from the light transport section 14. Exemplary components which may be used within the RFS optics suite 74 include, without limi-

tations, mirrors, positive lenses, negative lenses, acromats, compound lenses, astigmats, windows, flats, adaptive optics, holographical optical elements, spatial filters, pinholes, collimators, stages, wavelength filters, emission filters, and beam splitters.

As shown in FIG. 2, the fluorescence imaging module 34 includes a fluorescence imaging system 90 and a fluorescence image capture device 92. Exemplary fluorescence imaging systems 90 may include variety of optical components including, without limitation, microscopes, filter wheels, shutters, and optical filters. For example, green, yellow, and clear optical filters may be included. In one embodiment, the fluorescence imaging system 90 is configured to detect fluorescence from ultraviolet (UV) to infrared (IR) wavelengths. The fluorescence image capture device 92 may include a variety of devices including, without limitation, CCD chips and photomultiplier devices. Optionally, the fluorescence imaging module 34 may include a fluorescence optical suite 94 to refine or otherwise alter the light entering the fluorescence module 34. Exemplary components which may be used within the fluorescence optical suite 94 include, without limitations, mirrors, positive lenses, negative lenses, acromats, compound lenses, astigmats, windows, flats, adaptive optics, holographical optical elements, spatial filters, pinholes, collimators, stages, wavelength filters, emission filters, and beam splitters.

Referring again to FIG. 2, a beam director 98 may be included within or proximate to the analyzing section 12 and configured to direct light from the light transport section 14 to the OPS imaging module 30, the reflectance spectrophotometry module 32, and/or the fluorescence imaging module 34. Exemplary beam directors 98 include, without limitation, mirrors including dichroic mirror or elements and dark field mirrors, beam splitters, optical switches, movable or spinning geometric mirrors, corner cubes, prisms, and optical gratings. For example, in one embodiment the beam director 98 comprises a beam splitter directing fifty percent of the incoming light to the OPS imaging module 30 and 50 percent of the incoming light to the reflectance spectrophotometry module 32. In an alternate embodiment, the beam director 98 comprises a mirror having a non-reflecting area formed thereon, thereby reflecting a portion of light to the spectrophotometer and permitting dark field illumination to the OPS imaging module 30 and/or fluorescence imaging module 34. Optionally, the beam director 98 may comprise a spinning or moving mirrored polygon configured to reflect light from the light transport section 14 to the OPS imaging module 30, the reflectance spectrophotometer module 32, and/or the fluorescence imaging module 34. In another embodiment, the beam director 98 may be selectively actuated by the user to direct light to at least one of the OPS imaging module 30, the reflectance spectrophotometer module 32, the fluorescence imaging module 34, and/or any additional modules 34 coupled to or in optical communication with the analyzing section 12.

In one embodiment of the imaging system 10, the OPS imaging module 30 is coupled to the light transport section 14, while the reflectance spectrophotometer module 32 and/or the fluorescence imaging module 34 are positioned external to the imaging system 10 in optical communication therewith. A beam director 98 is positioned within the OPS module 30 and configured to direct a percentage (e.g. fifty percent) of the light received by the analyzing section 12 along an optical path to the reflectance spectrophotometer module 32 and the fluorescence imaging module 34, while the remaining light is directed to the OPS imaging module 30. An external beam director (not shown) may be used to further divide the

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directed light between the reflectance spectrophotometer module 32 and the fluorescence imaging module 34.

FIGS. 1 and 3 show an embodiment of a light transport section 14 of an imaging system 10. In the illustrated embodiment, the light source 20 is positioned proximate to a first lens 100. A variety of light sources may be used to illuminate the examination substrate 16, including, without limitation, incandescent lamps, gas discharge lamps, dye lasers, solid state devices such as light emitting diodes, laser diodes, gas lasers, excimer lasers, solid states lasers, and chemical lasers. For example, in one embodiment the external light source 20 comprises an incandescent lamp configured to irradiate the examination surface 16 with white light. In an alternate embodiment, the external light source 20 comprises a mercury lamp thereby stimulating fluorescence in the tissue of the examination substrate 16. In still another embodiment, the light source 20 comprises one or more LEDs configured to illuminate the examination substrate 16 with light of a discrete wavelength. In still another embodiment, the light transport section 14 may include a number of light sources. For example, a white light source and a UV light source could be used simultaneously. When using multiple light sources a shutter or beam splitter may be used to operate the system with a desired light source. For example, to operate the system using the white light source a shutter could be positioned to prevent the UV light from entering the light transport section 14. Thereafter, the user may actuate the shutter to illuminate the examination substrate 16 with the UV light rather than white light. In an alternate embodiment, a laser source may be coupled to or in optical communication with the imaging system 10 to treat the examination substrate 16. For example, the laser source may be used to treat microcirculatory disorders including, without limitation, cancerous tissue, skin discolorations, and/or tissue lesions. Optionally, the imaging system 10 may be operated without a first lens 100.

Referring again to FIGS. 1 and 3, light emitted by the external light source 20 is incident on a polarizer 102 configured to polarize light to a desired orientation. Thereafter, polarized light rays 104A, 104B, and 104C are incident on a light director 106 configured to direct light rays 104A', and 104B' to the examination substrate 16. In the illustrated embodiment, the light director 106 includes a non-reflective or dark field spot 108 formed thereon, thereby permitting light ray 104C to proceed therethrough and be absorbed by a beam dump or absorber 110. Exemplary light directors include, without limitation, beam splitters, dichroic junctions, and mirrors.

A light guide 112 in optical communication with the light source 20 receives and transmits light rays 104A', 104B' to the examination substrate 16. In the embodiment illustrated in FIG. 3, the light guide 112 includes an illumination segment 114 and a reflectance segment 116. The illumination segment 114 transmits light to the examination substrate 16 for illumination, while the reflectance segment 116 transmits reflected light from the examination substrate 16 to the beam director 98 of the analyzing section 12. Exemplary light guides include, for example, boroscopes, endoscopes, liquid light guides, polymer light guides, glass light guides, tubular bodies, and single or bundled optical fibers. For example, FIGS. 4A-4D show several embodiments of light guides 112 which may be used with in the light transport section 14. As shown in FIG. 4A, the light guide 112 may include polymer illumination and reflectance segments 114, 116, respectively. The reflectance segment 116 may be optically isolated from the illumination segment 114, for example, by an internal cladding 115. Similarly, the illumination segment 114 may

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include an external cladding 117 thereon. As shown in FIG. 4B, the reflectance segment 116 may be comprised of a bundle of optical fibers while the illumination segment 114 comprises a polymer light guide. In the alternative, FIG. 4C shows a light guide 112 having an illumination segment 114 constructed of a bundle of optical fibers and having a polymer reflectance segment 116 therein. FIG. 4D shows another embodiment wherein the illumination segment 114 and the reflectance segment 116 are constructed from a bundle of optical fibers.

As shown in FIG. 3, a lens or lens system 118 may be included within the light transport section 14 to focus the light rays 104A', 104B'. The focal point 120 of the lens system 118 may be located above, at the surface of, or below the surface of the examination substrate 16. Optionally, the lens system 118 may include a reflector or other device configured to project illuminating light at any angle relative to the longitudinal axis of the light transport body 14. For example, the lens system 118 may permit a user to project light at an angle of about 90 degrees relative to the longitudinal axis of the light transport body 14. As shown, the distal tip 137 of the light transport body 14 is positioned a distance D from the examination substrate 16. As a result, the light transport body 14 does not contact the examination substrate 16 thereby permitting the unimpeded flow of material through the examination substrate 16. As such, the imaging system 10 permits the user to measure the flow of a material through the examination substrate 16 in real time. Light 122 reflected from the examination substrate 16 is captured by the lens 118 and transmitted through the reflectance segment 116 and the dark field spot 108 of the light director 106 to the beam director 98 analyzing section 12. Optionally, a polarizer (not shown) may be positioned proximate to the distal tip 137 of the light transport body 14 and configured to polarize light prior to illuminating the examination substrate 16.

FIG. 5 shows an alternate embodiment of a light transport section 14. As shown, an internal light source 18 may be used to illuminate the examination substrate 16. For example, one or more LEDs may be used to illuminate an examination substrate 16 with a discrete wavelength of light. In an alternate embodiment, the internal light source 18 may comprise LEDs of different color, thereby illuminating the examination substrate 16 with light of multiple discrete wavelengths or with full spectrum light for additional treatment (e.g. laser ablation). Multiple wavelength LED's can also be used to generate images of the distribution of Hb saturation in an SDF imaging modality. Those skilled in the art will appreciate that the use of LEDs as a light source enables the imaging system 10 to be powered by a battery or other low-power power supply relative to previous systems. For example, the imaging system 10 may be powered by coupling the imaging system 10 to a universal serial port of a personal computer. One or more internal lenses 130 may, but need not be, included within the light transport section 14 and positioned proximate to the internal light source 18. Similarly, one or more optical polarizers or filters 132 may be positioned proximate to the internal lenses 130. The internal light sources 18 emit rays 134A, 134B which are transmitted to the examination substrate 16 by the illumination segment 136 of the light guide 138. An examination lens system 140 may be used to focus the light rays 134A, 134B to the examination substrate 16. A focal point 142 of the lens system 140 may be located above, at the surface of, or below the surface of the examination substrate 16. Thereafter, light rays 144 reflected by the examination substrate 16 are collected by the lens system 140 and

transmitted to the beam director **98** of the analyzing section **12** by the reflectance segment **146** formed within the light guide **138**.

FIG. **6** shows an alternate embodiment of a light guide **150**. As shown, the light guide **150** includes an illuminating segment **152** having a focused or curved distal tip **154**, thereby directing light rays to a focal point within an examination substrate (not shown). The reflectance segment **156** is configured to transmit light from the examination substrate **16** to the analyzing section **12** (See FIG. **1**).

FIGS. **7** and **8** show embodiments of spacer devices which may be affixed to the distal end or distal section of the light guide. FIG. **7** shows a light guide **160** having a spacer **162** attached thereto. In the illustrated embodiment, the distal section of the light guide **160** may include one or more lock members **164** thereon to securely couple the spacer **164** to the light guide **160**. As such, the spacer **160** may include a locking member recess **166** to accommodate the locking members **164**. The spacer **162** ensures that the light guide **160** remains at least a distance *d* from the examination substrate **16**. FIG. **8** shows an alternate embodiment of a spacer **172** coupled to a light guide **170**. The spacers **162**, **172** may be manufactured from a variety of materials including, without limitation, plastic, rubber, elastomer, silicon, or any other biologically compatible material. In one embodiment, the spacer **162**, **172** are disposable.

FIGS. **9** and **10** show an embodiment of a light guide **180** having an alternate embodiment of a spacer **182** attached thereto. The spacer **182** includes a vacuum port **184** attachable to a source of vacuum (not shown). The spacer **182** includes a spacer aperture **186** for irradiating the examination substrate (not shown). The spacer **182** includes one or more attachment orifices **188** thereon which are in communication with the vacuum port **184**. The attachment orifices **188** are formed between an exterior wall **190** and an interior wall **192** of the spacer body **194** and are isolated from the spacer aperture **186**. As such, the spacer **180** is configured to couple to the examination substrate (not shown) when the vacuum source is actuated without adversely effecting the irradiation of the examination surface. As such, the spacer **180** may be rigid or, in the alternative, may be constructed of a compliant material for use within or on compliant organs or structures. Like the embodiments described above, the spacer **182** may be manufactured from a variety of materials and may be disposable. One or more additional ports may be formed on the spacer body **194** for the administration of medicinal or therapeutic agents.

FIGS. **11** and **12** show an embodiment of an imaging system **200**. As shown, the imaging system **200** includes an illumination body **202** and a reflectance body **204**. The illumination body **202** defines an optics recess **206** configured to receive an optical system **208** therein. The optical system **208** includes a first spacer **210**, a first dark field mirror **212**, a filter spacer **213**, and a filter bank **214**. In the illustrated embodiment, the filter bank **214** includes a clear filter **216**, a yellow filter, **218**, a green filter **220**, and a white filter **222**. A second spacer **224** is positioned proximate to the filter bank **214**. A third spacer **226** is positioned between the second spacer **224** and a lens **228**. A fourth, fifth, and sixth spacers **230**, **232**, and **234**, respectively, are positioned proximate thereto. A second dark field filter **236** is positioned between the sixth spacer **234** and the seventh spacer **238**.

Referring again to FIG. **11**, the reflectance body **204** includes a light reflector **240** therein. The light reflector **240** includes a non-reflective area **242** formed thereon. In addition, the reflectance body **204** includes an examination tip **244** which is configured to be positioned proximate to the exami-

nation substrate (not shown). A polarizer and/or filter **246** and an image capture device **248** may be positioned within the analyzing section **250** of the reflectance body **204**. During use, a light source **252** projects light which is filtered and focused by the optical system **208** located within the illumination body **202**. The light from the light source **252** is directed by the light reflector **240** to the examination substrate (not shown) located proximate to the examination tip **244**. Light reflected by the examination substrate (not shown) is transmitted to the analyzing section **250** by the light guide **256**, where the light is depolarized and analyzed.

FIG. **13** shows another embodiment of an imaging system. As shown, the imaging system **300** includes an illumination body **302** and a reflectance body **304**. The illumination body **302** defines an optics recess **306** configured to receive an optical system **308** therein. The optical system **308** includes a first lens **310** and a second lens **312**. Positioned proximate to the first lens **310** is an internal light source **318**. In the illustrated embodiment, the internal light source **318** comprises a number of LEDs configured to project light through the optical system **308**. One or more reflectors **316** may be used to ensure that the light is transmitted through the illumination body **302**.

As shown in FIG. **13**, the reflectance body **304** includes a light reflector **340** therein. The light reflector **340** includes a non-reflective area **342** formed thereon. In addition, the reflectance body **304** includes an examination tip **344** which is configured to be positioned proximate to the examination substrate (not shown). A beam director **398** and an image capture device **348** may be positioned within the analyzing section **350** of the reflectance body **304**. During use, the light source **318** projects light which is focused by the optical system **308** located within the illumination body **302**. The light from the light source **318** is directed by the light reflector **340** to the examination substrate (not shown) located proximate to the examination tip **344**. Light reflected by the examination substrate (not shown) is transmitted to the analyzing section **350** by the light guide **356**, where the light is analyzed. As shown, the analyzing section **350** may include one or more filters or polarizers **360** therein.

As shown in FIGS. **3-5**, at least one light source may be used to illuminate structures located below the surface of a substrate. FIGS. **14** and **15** show alternate embodiments of imaging systems useful in imaging sub-surface structures while avoiding or reducing the effects of surface reflection. FIG. **14** shows an imaging system **400** comprising a body **402** having one or more imaging passages **404** formed therein. One or more illumination passages **406** may be formed within the body **402** and may be optically isolated from the imaging passage **404**. In one embodiment, the body is rigid. In an alternate embodiment, the body **402** is flexible. For example, the body **402** may comprise a catheter body. Optionally, the body **402** may include an additional lumen formed therein. For example, an additional lumen may be positioned within the body **402** and may be used to deliver therapeutic agents to a treatment site. In another embodiment, an additional lumen may be used to deliver a vacuum force to a treatment site. In the illustrated embodiment, the illumination passage **406** is positioned radially about imaging passage **404**. In the illustrated embodiment, the illumination passage **406** encircles the imaging passage **404**. In an alternate embodiment, the illumination passage **406** may be positioned anywhere within the body **402**. As shown, the illumination passage **406** is optically isolated from the imaging passage **404**. Therefore, illuminating energy transported through the illumination passage **406** is prevented from entering the imaging passage **404**. As such, the present systems permit side stream dark field

imaging (hereinafter SDF). As shown in FIG. 14, a feature of SDF imaging is that the illuminated light **412A** and **412B** and the reflected light **414** travel via independent pathways. Thus, the illumination can be placed directly on the tissue and the observations can be made adjacent to it without light crossing over between two paths.

Referring again to FIG. 14, at least one illumination source may be positioned within the illumination passage **406**. In one embodiment, the illumination source **410** comprises one or more LED's configured to project a selected wavelength to the substrate **420**. In an alternate embodiment, the illumination source **410** comprises a plurality of LED's configured to project multiple wavelengths to the substrate **420**. For example, as shown in FIG. 14 a first illumination source **410A** configured to project light to the substrate **420** is positioned at the distal portion **418** of the body **402**. Similarly, a second illumination source **410B** is positioned at the distal portion **418** of the body **402**. As such, the first and second illumination sources **410A**, **410B** are positioned proximate to the substrate **420** under examination. Optionally, any number of illumination sources may be positioned within the body **402**. Exemplary illumination sources include, without limitation, LED's, LLED's, incandescent bulbs, laser light sources, etc.

FIG. 15 shows a perspective view of the distal portion of an alternate embodiment of the imaging device **400** shown in FIG. 14. As shown, the body **402** includes an imaging passage **404** and at least one illumination passage **406** optically isolated from the imaging passage **404**. One or more illumination devices **410** are located within the illumination passage **406** and positioned proximate to the distal portion **418** of the body **402**. As such, during use the illumination source are positioned proximate to the substrate **420**.

FIG. 16 shows a cross sectional view of the distal portion of an embodiment of an imaging device. As shown, The body **402** defines an imaging passage **404** and an illumination passage **406** therein. Like the previous embodiments, the illumination passage **406** is optically isolated from the imaging passage **404**. In the illustrated embodiment, the illumination passage **406** terminates proximate to the distal portion **418** of the body **402**. Optionally, the illumination passage **406** may continue through the length of the body **402**. As such, the illumination passage **406** may include one or more optical fibers configured to deliver illuminating energy to the substrate **420** from a remote location. In the illustrated embodiment, one or more illumination sources **410** are positioned within the illumination passage **406**. For example, one or more LED's may be positioned within the illumination passage **406**. Like the previous embodiments shown in FIGS. 14 and 15, the illumination passage **406** is optically isolated from the imaging passage **404**. Optionally, at least one conduit **424** may traverse through the body **402** thereby coupling the illumination source **410** to a source of power. In the illustrated embodiment at least one lens **422** is positioned within the imaging passage **404** thereby transmitting an image received from a substrate **420** to an image capture device **416**. (See FIG. 14). Optionally, the imaging system shown in FIGS. 14-16 may be used without a lens **422**.

With reference to FIG. 14, during use, the first illumination source **410A** projects illuminating energy **412A** to the substrate **420**. Similarly, the second illumination source **410B** projects illuminating energy **412B** to the substrate **420**. As shown in FIG. 14, the illumination energies **412A**, **412B** are optically isolated from the imaging passage **404**. The first and second illumination energies **412A**, **412B** may be the same or differing wavelengths. Further, as the first and second illumination sources **410A**, **410B** are positioned at the distal portion of the body **402** proximate to the substrate **420**, surface reflec-

tions therefrom are reduced or eliminated. As shown, a sub-surface image **414** is transported by the imaging passage **404** from the substrate **420** to an image capture device **416**. Exemplary image capture devices include, without limitation, CCD devices, cameras, spectrophotometers, photomultiplier devices, analyzers, computers, etc. Optionally, one or more lenses **422** may be positioned within the image passage **404** or body **402** to focus illumination energy **412** to the substrate **420** or to assist in the transport of an image **414** from the substrate **420** to the image capture device **416**, or both. As stated above, the optical isolation of the illumination energy from the image received from the substrate reduces or eliminates the effects of surface reflections while enabling SDF imaging in addition to a variety of alternate imaging modalities or spectroscopic examination of an area.

FIG. 17 shows an alternate embodiment of an SDF imaging system. As shown, the SDF imaging system **450** comprises a body **452** defining an imaging passage **454** and an illumination passage **456** optically isolated from the imaging passage **454**. The illumination passage **456** includes one or more illumination sources **460** therein. Exemplary illumination sources **460** include, without limitation, LED's, LLEDs, and incandescent bulbs. As shown, the illumination sources **460** are located proximate to the distal portion **462** of the body **452**. Optionally, the illumination sources **460** may be located some distance from the examination area. As such, illuminating energy may be transported to the examination area through fiber optic conduits positioned within the body **452**. Like the previous embodiments, the body **402** may be rigid or flexible. In the illustrated embodiment, a cap device **464** is positioned over the body **452**. In one embodiment, the cap device **464** may comprise an optically transparent disposable cap device **464** configured to be detachably coupled to the body **452**. During use the cap device **464** may protect the body **402** from biological materials and contaminants. As such, the cap device **464** may be sterile.

Referring again to FIG. 17, at least one lens **466** may be positioned within the imaging passage **454**. The imaging passage **454** is in optical communication with an imaging capture device **468**. The image capture device **468** may comprise any of devices useful in capturing and analyzing an image received from a substrate. For example, the image capture device **468** may comprise a CCD device, photomultiplier, computer, spectrophotometer, and the like. Further, a focusing device **470** may be included within the body **452** or the image capture device **468**. Exemplary focusing devices include, without limitation, additional lenses, mechanical drives or positioners, and the like. Optionally, the SDF imaging system **450** may further include a handle **472** to assist a user in positioning the device. Further, the SDF imaging system **450** may be configured to be coupled to a computer, power source, etc.

FIG. 18 shows an alternate embodiment of an imaging system. As shown, the imaging system **500** includes a body **502** defining an imaging passage **504** and at least one illumination passage **506** optically isolated from the imaging passage **504**. The illumination passage **506** includes one or more illumination sources **510** therein. As shown, the illumination sources **510** are located proximate to the distal portion **518** of the body **502**, however, the illumination source may be located anywhere on the body **502**. Optionally, a cap device (not shown) may be positioned over the body **502**. For example, the cap device (not shown) may comprise an optically transparent disposable device configured to be detachably coupled to the body **502**.

Referring again to FIG. 18, at least one lens **522** may be positioned within the imaging passage **504**. The imaging

passage 504 is in optical communication with at least one image capture device 516. In the illustrated embodiment, a first image capture device 516A and a second image capture device 516B may be used with the system. Further, one or more optical modulators 526 may be positioned within the image passage 504 and configured to modulate imaging signals from the substrate 520. exemplary optical modulators 526 include, without limitation, mirrors, band pass plates, polarizers, gratings, and the like. The image capture devices 516A, 516B may comprise any number of devices useful in capturing and analyzing an image received from a substrate. For example, the image capture devices 516A, 516B may comprise CCD devices, spectrophotometers, spectrum analyzers, and the like.

As shown in the FIGS. 18 and 19, the illumination sources 510 may comprise LEDs of a single wavelength. In the alternative, the illumination sources 510 may be configured to irradiate light of multiple wavelengths. For example, FIG. 19 shows a device having a first illumination source 510A irradiating at a first wavelength and a second illumination source 510B irradiating at a second wavelength. FIG. 20 shows a device having a first illumination source 510A, a second illumination source 510B, and a third illumination source 510C, each illumination source irradiating at a different wavelength. As such, the system may be configured to perform a number of imaging and analyzing procedures with a single device. For example, a first wavelength may be projected to the substrate and used for SDF microcirculation imaging within the underlying vasculature, while a second wavelength may be projected to the substrate and used for detecting oxygen saturation within a blood flow. In short any number of wavelengths of illuminating energy may be projected from the illumination sources 510 and used for any number of analytical processes. For example, the imaging system 500 may be configured to permit imaging of the microcirculation and spectroscopic examination of an area with a single device.

Referring to FIGS. 18 and 21, during use the distal portion 518 of the body 502 may be in contact with the substrate 520 under examination. As such, the illumination source(s) 510 may be positioned in close proximity to the substrate 520. Optionally, the distal portion 518 may include one or more engaging devices 528 coupled to the body 504 or the cap device (not shown). For example, as shown in FIG. 22, the engaging device 528 may comprise an inflatable device configured to dissipate a pressure applied to the substrate 520 by the distal portion 518 of the body 502. In an alternate embodiment, shown in FIG. 23, the distal portion 518 may be positioned proximate to, but not in contact with, the substrate 520. As such, the illumination sources 510 may be configured to project illuminating energy 512A, 512B to the substrate 520. Optionally, one or more lenses may be in optical communication with the illumination source(s) 510 to aid in the projection of illumination energy 512A, 512B to the substrate 520.

FIG. 24 shows a block diagram of an embodiment of an imaging and analyzing system. As shown, the imaging system 600 includes an analyzing section 602, a light transport section 604, and a light delivery section 606 configured to deliver light to and receive information from a substrate 608. As stated above, the analyzing section 602 may include any number of analyzing modules configured to process information received from the substrate 608. In the illustrated embodiment, the analyzing section 602 includes an OPS imaging module 620, a dark field illumination module 622, a reflectance spectrophotometry module 624, an additional processor module 626, a fluorescence module 628, and/or a

fluorescence lifetime module 630. The additional processor module 626 may include one more processing module including, without limitation, Raman spectroscopy devices, fluorescence decay processors, PpIX analyzers, and/or OCT (Hb sat) analyzers, and/or CO2 analyzers. Referring to FIGS. 18 and 21, the analyzing section 602 may be configured to receive imaging information from the substrate 520 via the imaging passage 504 formed within the body 502. Those skilled in the art will appreciate that the present system enables a user to selectively analyze a substrate using multiple imaging modalities, spectrophotometry modalities, and similar analyzing methods using a single device coupled to multiple analyzers.

The light transport section 604 may comprise a body 632 configured to transport light to and from the substrate 608. For example, the body 632 may include an image passage 504 and an optically isolated illumination passage 506 as shown in FIG. 18. Further, the light transport section 604 may include one or more internal illumination sources 636 positioned therein and configured to irradiate the substrate 608. Optionally, one or more optical elements 634 may be positioned within the body 632. Further, the body 632 may be configured to receive and transport light from an external light source 638 to the substrate 608.

Referring again to FIG. 24, the light delivery section 606 may comprise a direct illumination source 640 configured to be positioned proximate to the substrate 608 and providing direct illumination thereto. As such, the direct illumination source 640 is optically isolated from an image received from the substrate 608. Exemplary direct illumination sources 640 include LLED's, LED's, and the like. Further, one or more white light illumination sources 642 may be used to illuminate the substrate 608. In one embodiment, the light delivery section 606 may be configured to deliver materials to or receive materials 644 from the substrate 608. For example, the light delivery section 606 may be configured to infuse therapeutic agents to the substrate 608. Optionally, the light delivery section 606 may include one or more engaging devices 646 positioned thereon to assist in positioning the system during use.

As stated above, the preceding imaging and analyzing systems disclosed herein may include one or more cap devices 464 which may be detachably coupled to the body 452. (See FIG. 17). Generally, the cap device 464 may comprise optically transparent materials configured to protect the body 452 during use. As such, the cap device 464 may be disposable. FIG. 25 shows an alternate embodiment of a cap device 714. As shown in FIG. 25, the imaging device 700 includes a body 702 having an imaging passage 704 and an illumination passage 706 optically isolated from the imaging passage 704 formed therein. The illumination passage 706 may include one or more conduits 708 coupled to one or more illumination sources 710 located therein. As shown in FIG. 25, one or more lenses 712 may be positioned within the imaging passage 704. A cap device 714 may be coupled to the body 702. The cap device 714 includes an illumination field 716 optically isolated from an imaging relief 718. In the illustrated embodiment, the illumination field 716 is positioned proximate to the illumination sources 710 located within the body 702. Similarly, the imaging relief 718 is positioned proximate to the imaging passage 704. At least one isolation surface 720 optically isolates the illumination field 716 from the imaging relief 718. For example, in the illustrated embodiment the isolation surface 720 include a reflective foil 722 thereon which is configured to prevent light from illumination sources 710 from directly entering the imaging passage 704 without first engaging a substrate under examination. Alternate isola-

tion materials may be used on the isolation surface **720** including, without limitation, dyes, foils, impregnations, etc. Optionally, the cap device **714** may be disposable and may be configured to detachably couple to the body **702**.

FIG. **26** shows yet another embodiment of a reflectance avoidance imaging system. As shown, the reflectance avoidance imaging system **810** includes an imaging device **812** having a spacer or tissue engaging tip **814** attached thereto. The imaging device **812** includes a body **816** having a distal portion **818** configured to receive and engage the spacer **814**. In one embodiment, the spacer **814** is detachably coupled to the body **816**. Optionally, the spacer **814** may be non-detachably coupled to the body **816**.

Referring again to FIG. **26**, the imaging body **816** includes one or more conduits formed therein. In the illustrated embodiment, the body **816** includes an imaging conduit **820** configured to project light from a light source (not shown) to a work surface. In addition, the imaging conduit **820** collects light reflected from the work surface and transports the reflected light to a sensor suite (not shown) in communication therewith. Exemplary sensor suites include, without limitation, a CCD or any other type of imaging or sensing device, spectral photometers, and the like. Optionally, a secondary imaging conduit **822** may be positioned within the body **816**. For example, the secondary imaging conduit **822** may be configured to measure CO₂ within tissue through the use of a CO₂ sensing dye. The CO₂ sensing dye enables the measurement of fluorescence decay and may utilize light received from and transmitted through the imaging conduit **820**. Optionally, one or more additional conduits **824** may be positioned within the body **816**. For example, any number of fluid conduits may be formed within the body **816**.

The spacer **814** includes a spacer body **830** having a coupling portion **832** configured to engage and couple the distal portion **818** of the body **816**. The spacer body **830** further defines an orifice **834** which is in communication with the coupling portion **832**. In the illustrated embodiment, the spacer body **830** includes thread members **836** and attachment devices **838** formed or otherwise disposed thereon to enable the spacer body **830** to couple to the body **816**. Any number or type of thread members **836** and attachment devices **838** may be used to couple the spacer body **830** to the imaging device **812**. The distal portion of the spacer body **830** includes a flange **840** defining the orifice **834**. In the illustrated embodiment, the flange **840** includes one or more vacuum ports **842** portioned thereon, thereby permitting the flange **840** to engage or couple to the a work surface.

In the illustrated embodiment, the spacer **814** includes one or more vacuum ports **842** which enable the spacer **814** to engage the work surface. Optionally, the spacer body **814** may be configured to avoid contacting the work surface. For example, the spacer body **814** may include an optical system comprised of one or more lenses to enable the imaging device **812** to project and receive light to and from a work surface from a distance without contacting the work surface. For example the optical system may include a zoom lens system.

Further, the spacer **814** may be formed in any variety of shapes and size. For example, the spacer may include a doughnut-shaped spaces. Furthermore, the spacer **814** may include a bladder or cushion filled with any variety of fluids. Optionally, the fluid may be optically transparent.

FIG. **27** shows a cross sectional view of an embodiment of a reflectance avoidance imaging system **810**. As shown, the body **816** includes the imaging conduit **820**, the secondary imaging conduit **822**, and the addition conduit **824** formed therein. In addition, vacuum conduits **856** and **858** are formed within the body **816** and a couple to a vacuum source (not

shown). The spacer **814** includes vacuum conduits **870** and **872** which are in communication with the vacuum conduits **856** and **858** of the body **816** and the vacuum ports **842** formed on the spacer **814**. Optionally, one or more attachment members **862** may be positioned on the body **816** to further enable coupling of the spacer **814** to the body **816**.

In addition to the novel imaging devices described above, the present application describes a method of imaging and determining various biological parameters non-invasively and, if needed, treating an affected area. For example, when operating the above-described system in an OPS imaging mode, flow through the capillaries and related circulatory structures may be examined by viewing red blood flow there-through. To operate the system in an OPS imaging mode, the user irradiates the examination substrate with white light. The white light is polarized by a polarizer prior to illuminating the examination substrate. Reflected light is captured by the light guide and transmitted to the polarizing section **42** of the OPS imaging module **30** (See FIG. **2**). Light reflected by the system optics and the patient's tissue surface undergoes a polarization shift as a function of scattering and, thus, is cancelled by the polarizing section **42**. As such, sub-surface reflected light fails to undergo a polarization shift and will be captured by the image capture device **50**, thereby enabling sub-surface imaging. Optionally, OPS imaging may be accomplished in combination with dark field illumination.

Similarly, the imaging system described herein may be used to perform reflectance spectrophotometry using the reflectance spectrophotometry module. A spectrophotometer may be used with the present imaging system to examine the spectral reflectance of the tissue surface. Light from a light source illuminates an examination substrate. The light may comprise an internal light source **18**, external light source **20**, and/or an ancillary light source **22**. (See FIG. **1**). Light reflected by the examination substrate **16** is captured by a light transport section **14** and transmitted to a reflectance spectrophotometry module. The spectral characteristic of the reflected light may then be examined and used to determine the hemoglobin saturation, and/or hematocrit concentration within the surface of an organ under investigation.

Lastly, the imaging system described herein may be used to determine the oxygenation and/or functional state of a tissue cell using the fluorescence imaging module. For example, an examination area may be illuminated with UV light thereby targeting the mitochondrial energy state therein. For example, light having a wavelength of about 360 nm may be used to illuminate the examination substrate. Thereafter, light reflected by the substrate may be captured by the light transport section **14** and transmitted to the analyzing section **12**. (See FIG. **1**) The captured light may undergo a lambda shift from 360 nm to about 460 nm. Thereafter, a fluorescence imaging module **34** may analyze the reflected light for to determine the presence of NADH in the cells, thereby showing availability of oxygen within the cells.

The OPS imaging processor **52**, RFS processor **72**, and fluorescence imaging processor **92** may each contain any number of formulas, algorithms, models, databases, look-up tables, or related information to compute and display their respective reflectance measurements. For example, Beers-Lambert law may be used to determine the concentration of material in the examination substrate based on the absorbance of the light by the examination substrate.

Also disclosed herein is a method of comprehensively monitoring the microcirculation of a patient. The method may include using any of the aforementioned imaging systems disclosed herein. In one embodiment, the method includes illuminating a tissue substrate, avoiding the reflection of light

from the surface of the tissue substrate, receiving light from the tissue substrate, utilizing some of the received light to image microcirculatory flow in the tissue substrate, utilizing some of the received light to determine oxygen availability in the microcirculation, and utilizing some of the received light to determine the adequacy of oxygenation of the tissue cells.

In one embodiment, the aforementioned method may include utilizing the microcirculatory flow information, the oxygen availability information, and the adequacy of oxygenation of tissue cells information, making an early and sensitive determination regarding states of shock, such as septic, hypovolemic, cardiogenic and obstructive septic shock, in patients, and guiding resuscitation therapies aimed at correcting this condition.

In another embodiment the aforementioned method may also include utilizing the microcirculatory flow information, the oxygen availability information, and the adequacy of oxygenation of tissue cells information, and making an early and sensitive determination regarding cardiovascular disease and failure of the patient.

Any of the embodiments of the imaging systems and methods discussed herein may also include pulsed lighting systems and techniques to enhance the output quality of elements of the system such as the resolution of video output images. FIG. 28 shows a block diagram of an embodiment of an imaging system 600A similar to the imaging system 600 shown in FIG. 24. Imaging system 600A includes synchronized pulsed lighting controlled by controller 900. The synchronized pulsed lighting may be used for imaging a substrate, such as a biological substrate including skin, blood vessels, internal organs or the like, in order to observe or analyze biological metrics such as microcirculation within a structure. In some embodiments, light reflected from an examination substrate may be analyzed with a high resolution video output image, even where object or objects of the substrate being imaged are moving across the field of view.

The controller 900 may include a processor configured to accept video synchronization data from an imaging system, such as a CCD camera control system (not shown) and generate an output signal to pulse one or more of the lighting elements of the imaging system 600A, or any other suitable imaging system embodiment, in a desired manner. As shown in FIG. 24, the controller 900 is in communication with the analyzing section 602 and one or more of the light systems 636, 638, 640 and 642. Although the controller 900 is shown in communication with the analyzing section 602 as a whole, the controller may be in specific communication, such as electrical or optical communication, with any of the elements of the analyzing section 602. The controller may be in specific communication with the fluorescence lifetime CO₂ module 630, the fluorescence imaging module 628, the reflectance spectrophotometry RS module 624 and the additional modules 626. Although the controller 900 is shown as a separate element of the system 600A, the controller 900 may be disposed within or otherwise incorporated into other elements of the system 600A such as the analyzing section 602, the light transport section 604, the light delivery section 606, or any sub-component thereof.

The controller may also be in specific communication with the DF imaging module 622 or the OPS imaging module 620 which may include, for some embodiments, a video device such as a video CCD camera. This arrangement may be of particular use where the target or object of imaging by these modules is moving across the imaging field. Many commercially available CCD video cameras utilize a CCD chip that includes a grid or array of pixels that gather or integrate image light over a period of time in order to achieve sufficient

sensitivity to capture image light in normal lighting conditions. Once integrated, the light information is communicated or otherwise output to a display system where it is converted to a signal that can be displayed on a monitor or the like. In order to comply with video output conformance standards, such as NTSC standards, the pixel array is divided into sets or lines. For some embodiments, these sets may include odd and even horizontal line sets, particularly for a system that uses the interlacing method of integrating the field lines.

With respect to such a video imaging system using continuous lighting to illuminate the target substrate or object, each interlaced image consists of an odd and an even field, containing the odd and even lines. Under normal operating conditions 30 images (25 for European standard) are generated each second. Thus the video signal consists of 30 even and 30 odd fields separated by $\frac{1}{60}$ second. FIG. 29 illustrates a diagrammatic view of a video capture sequence in an interlaced frame integration system. As shown in FIG. 29, the odd field integrates its signal from the end or output point of the previous odd field until the moment the integrated odd field light data is output, i.e. during $\frac{1}{30}$ second, as shown by ramp FIG. 902. The even field integrates its signal from the end or output point of the previous even field until the moment it is output, as shown by ramp FIG. 904. The ramp FIGS. 902 and 904 represent an increased data acquisition over time until the end of the interval when the data is output and the process starts over.

Thus, both the odd and even fields integrate over equal intervals or periods of time but with the start of the intervals separated or staggered by $\frac{1}{60}$ second. As a result there is a slight difference in the moment the two fields, that belong to the same image, are illuminated. When imaging a moving object, the odd-lines of an output image may not spatially match, or may otherwise be displaced with respect to, the even lines of the output image. This is shown in FIG. 30 which illustrates a diagrammatic view of a video image of a substantially round object 906 taken with a typical video system, such as a Sony® system, using frame integration where the object is moving across the field and the output image 906 is blurred as a result of the movement and use of a continuous or substantially continuous illumination light or LED. The blurring is a result of the relative displacement between the output display of the odd lines 908 with respect to the output display of the even lines 910.

In order to maintain a high level of image resolution, the blurring discussed above can be reduced or eliminated by pulsing the illumination lighting of the imaging subject. For example, some embodiments of the imaging system 600A may be equipped with a Sony® type video CCD-camera, such as a Sony XC® camera, manufactured by Sony Corporation® and may use a special lighting technique in which a light source, such as internal LED light source 636 or direct illumination LEDs 640, is pulsed synchronously with the video-signal of the CCD-camera. For some embodiments, an output signal from the video camera or device containing information about the timing of the internal image integration process of the video device is communicated to the controller 900 which is configured to then generate a synchronized pulsed signal to power the light source, such as internal LED light source 636, direct illumination LEDs 640 or the like. As a result, the sharpness of the image 906 of moving objects (e.g. erythrocytes) may be improved and differences in the moment of illumination of the odd lines 908 and even lines 910 of the image are absent, further improving the image quality. For example, deeper imaging penetration of tissue is possible. Secondly, a morphological distinction between arterioles and other microstructures (including the micro-capil-

laries) can be made. This may allow pattern recognition software to be utilized to make these microstructure discriminations and therefore calculate relevant clinical parameters, i.e. micro-capillary density and/or blood flow in the capillaries.

FIG. 31 illustrates a diagrammatic view of a video image 912 of the same object as that of FIG. 30 but taken with synchronized pulse lighting. The image 912 shows a substantially round object moving across the field and wherein the output image 912 has no or substantially no blurring as a result of the movement. The image 912 illustrated in FIG. 31 may be generated by a pulsed LED 636 or 640, or any other suitable lighting element or source, which is on only during the interval in between the end of the integration of a previous even field (or start of integration of the present even field) and the start of the output (or end of integration) of the odd field. Such pulsing of the light source may be carried out for some embodiments, as discussed above, with an output signal from a video camera or similar device being processed by the controller 900 which is configured to generate a synchronized pulsed signal to the light source or sources. For the embodiment shown in FIG. 29, the interval from the start of the integration of the even field to the end of integration or moment of output of the odd field there is an interval having a length of $\frac{1}{60}$ second, denoted by the arrow T. During interval T, which corresponds to an overlap period for the integration of the odd and even fields, data integration of the odd and even fields is synchronized and the integration is carried out simultaneously. When restricting the illumination to this overlap interval or period, there is no time difference or spatial separation between the illumination and display of the odd and even field of an image.

For such an embodiment, the LED (or other type of lighting) is off during the interval between the odd and even fields, and thus, the duty-cycle of the lighting is about 50 percent for this embodiment. As a result the image is sharper (illuminated during $\frac{1}{60}$ second pulse-time instead of $\frac{1}{30}$ second integration time in the continuous mode) and the odd and even fields are illuminated at the same moment and odd and even lines match each other. In some embodiments, and particularly European formats, a video camera's image rate may be about 20 images per second to about 30 images per second, specifically, about 25 images per second. For such embodiments the interval between the odd and even fields may be about $\frac{1}{50}$ second, but otherwise, all of the methods discussed above with regard to pulsed synchronized lighting may be used.

With regard to the above detailed description, like reference numerals used therein refer to like elements that may have the same or similar dimensions, materials and configurations. While particular forms of embodiments have been illustrated and described, it will be apparent that various modifications can be made without departing from the spirit and scope of the embodiments of the invention. Accordingly, it is not intended that the invention be limited by the forgoing detailed description.

What is claimed is:

1. An imaging system for analyzing a tissue substrate, comprising;
 - a light source;
 - a light transport body configured to project light from the light source to the tissue substrate and transmit light from the tissue substrate;
 - an analysis section which is in optical communication with the light transport body and which includes a video imaging system that utilizes a plurality of sets of field lines integrated over staggered time intervals that over-

- lap in an overlap period for odd and even field lines that will be integrated into a single image; and
- a controller which is in communication with the light source and video imaging system and which is configured to activate the light source to emit a synchronized light pulse having a duty cycle of lighting of about 50% to be on only during the overlap period of odd and even field lines that will be integrated into a single image of the video imaging system.
2. The system of claim 1 wherein the analysis section further comprises a reflectance avoidance imaging module, a reflectance spectrophotometry module, an fluorescence imaging module and a beam director which is in optical communication with the light transport body and which is configured to direct at least a portion of the light from the tissue substrate to at least one of the reflectance avoidance imaging module, the reflectance spectrophotometry module, and the fluorescence imaging module.
3. The system of claim 2 wherein the beam director is configured to be selectively actuated by a user.
4. The system of claim 2 wherein the beam director comprises at least one device selected from the group consisting of a beam splitter, dichroic junction, prism, and mirror.
5. The system of claim 1 wherein the light transport body further comprises one or more illumination passages configured to project light from the light source and an imaging passage configured to transmit the light from the tissue substrate, wherein the imaging passage is optically isolated from the one or more illumination passages.
6. The system of claim 1 wherein the light source is selected from the group consisting of incandescent lamps, gas discharge lamps, light emitting diodes, laser diodes, gas lasers, excimer lasers, solid state lasers, chemical lasers, dye lasers, infrared sources, and UV sources.
7. The system of claim 1 further comprising a lens positioned within an imaging passage and wherein the imaging passage is in optical communication with the video imaging system.
8. The system of claim 7 further comprising one or more optical modulators positioned within the imaging passage.
9. The system of claim 1 wherein the duty cycle of lighting of about 50% comprises an interval of $\frac{1}{60}$ of a second.
10. An imaging system for analyzing a tissue substrate, comprising;
 - an LED light source;
 - a light transport body configured to project light from the LED light source to the tissue substrate from a side and transmit light from the tissue substrate;
 - an analysis section which is in optical communication with the light transport body, which is configured to receive light from the tissue substrate and which includes a reflectance avoidance imaging module, a reflectance spectrophotometry module, a fluorescence imaging module and a video imaging system that utilizes a plurality of sets of field lines integrated over staggered time intervals that overlap in an overlap period for odd and even field lines that will be integrated into a single image; and
 - a controller which is in communication with the LED light source and video imaging system and which is configured to synchronously pulse the LED light source so as to have a duty cycle of lighting of about 50% and to be on only during the overlap period of odd and even field lines that will be integrated into a single image of the video imaging system.
11. The system of claim 10 further comprising a beam director in optical communication with the light transport

body configured to direct at least a portion of the received light to at least one of the reflectance avoidance imaging module, the reflectance spectrophotometry module, and the fluorescence imaging module.

12. The system of claim 10 wherein the light transport body further comprises one or more illumination passages which are positioned radially around an imaging passage.

13. The system of claim 12 wherein the one or more illumination passages comprise one or more optical fibers configured to deliver illuminating energy from a remote location.

14. The system of claim 10 wherein the light transport body has a proximal end and a distal end and wherein the LED light source comprises one or more LED's positioned at the distal end of the light transport body.

15. The system of claim 10 further comprising an optically transparent disposable cap device configured to be detachably coupled to a distal end of the light transport body.

16. The system of claim 10 wherein the LED light source comprises LED's emitting a single light wavelength.

17. The system of claim 10 wherein the light transport body has a proximal end, a distal end and an engaging device disposed at the distal end of the light transport body.

18. The system of claim 17 wherein the engaging device comprises an inflatable device configured to dissipate a pressure applied to the tissue substrate.

19. The system of claim 10 wherein the duty cycle of lighting of about 50% comprises an interval of $\frac{1}{60}$ of a second.

20. A method of monitoring a patient, comprising:
 providing an imaging system including a light source, a light transport body configured to project light from the light source to tissue substrate and transmit light from the tissue substrate, an analysis section in optical communication with the light transport body and a video imaging system that utilizes a plurality of sets of field lines integrated over staggered time intervals that overlap in an overlap period for odd and even field lines that will be integrated into a single image and a controller configured to activate the light source so as to have a duty cycle of lighting of about 50% and only within the overlap period of odd and even field lines that will be integrated into a single image of the video imaging system; illuminating a tissue substrate of the patient over a duty cycle of lighting of about 50% with pulsed synchronized light from the light source only during an overlap period of odd and even field lines that will be integrated into a single image of the video imaging system; receiving light from below a surface of the tissue substrate; and

generating an image of the tissue substrate with the sets of field lines integrated during the overlap period.

21. The method of claim 20 wherein the tissue substrate comprises vascularized tissue and further comprising imaging microcirculation of the tissue and obtaining microcirculatory information.

22. The method of claim 21 further comprising:
 obtaining oxygen availability information, and adequacy of oxygenation of tissue cells information;
 making an early and sensitive determination regarding at least one state of shock in the patient; and
 using the information obtained to guide resuscitation therapies aimed at correcting a state of shock in the patient.

23. The method of claim 22 wherein obtaining adequacy of oxygenation of tissue cells information comprises measuring tissue CO₂ or NADH via fluorescence imaging.

24. The method of claim 22 wherein making an early and sensitive determination regarding at least one state of shock comprises making an early and sensitive determination regarding a state of shock selected from septic shock, hypovolemic shock, cardiogenic shock and obstructive septic shock, in the patient.

25. The method of claim 21 further comprising:
 obtaining oxygen availability information and an adequacy of oxygenation of tissue cells information; and
 making an early and sensitive determination regarding cardiovascular disease and cardiovascular failure of the patient.

26. The method of claim 20 further comprising illuminating the tissue substrate without influencing microcirculation of the tissue substrate.

27. The method of claim 20 further comprising reflectance filtering of the light received from below a surface of the tissue substrate that includes OPS imaging or Mainstream Dark Field imaging.

28. The method of claim 20 further comprising reflectance filtering of the light received from below a surface of the tissue substrate that includes Mainstream Dark Field imaging.

29. The method of claim 20 wherein illuminating the tissue substrate comprises sidestream dark field imaging wherein incident and light received from below a surface of the tissue substrate do not travel down a same pathway.

30. The method of claim 20 wherein illuminating a tissue substrate of the patient over a duty cycle of lighting of about 50% comprises illuminating a tissue substrate of the patient over an interval of $\frac{1}{60}$ of a second.

* * * * *

UNITED STATES PATENT AND TRADEMARK OFFICE
CERTIFICATE OF CORRECTION

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APPLICATION NO. : 11/288844
DATED : September 15, 2015
INVENTOR(S) : Can Ince and Theodorus Antonius Herman Maria Scholten

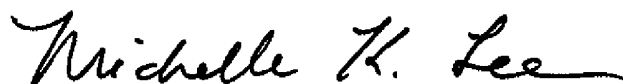
Page 1 of 1

It is certified that error appears in the above-identified patent and that said Letters Patent is hereby corrected as shown below:

Title page, inventors names should read:

(75) Inventors: Can INCE, Leiden (NL); Theodorus Antonius Herman Maria SCHOLTEN, Middelaar (NL)

Signed and Sealed this
Twenty-second Day of March, 2016



Michelle K. Lee
Director of the United States Patent and Trademark Office

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[标]发明人	INCE CAN SHOLTEN THEODORUS ANTONIUS HERMAN MARIA		
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CPC分类号	G02B21/084 G02B21/365 A61B5/0261 A61B1/00186 A61B1/042 A61B1/043 A61B1/06 A61B1/0607 A61B1/0646 A61B1/0684 A61B5/14556 A61B5/412 A61B1/0638 A61B5/0059 A61B3/1241 A61B5/0066		
优先权	60/632348 2004-11-30 US		
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外部链接	Espacenet USPTO		

摘要(译)

利用反射率避免以及其他成像模态监测患者的系统和方法。可以获得关于灌注，氧饱和度和氧气可用性的信息以及其他信息。系统实施例可包括光源，被配置为将光从光源投射到检查基板并透射由检查基板反射的光的光传输体，以及与光传输体光学连通的分析部分。光源可以是脉冲的，以便改善由系统产生的视频图像的质量。

