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(54) **PHYSIOLOGICAL MONITORING GARMENT**

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USPC ..... **600/301**; 600/372; 600/409; 600/529;  
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See application file for complete search history.

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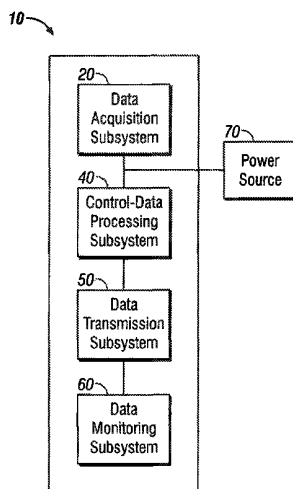
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(57) **ABSTRACT**

The present invention is directed to systems and methods for monitoring characteristics of a subject. A system according to an exemplary embodiment of the invention includes a sensor subsystem including at least one respiratory sensor disposed proximate to the subject and configured to detect a respiratory characteristic of the subject, wherein the sensor subsystem is configured to generate and transmit at least one respiratory signal representing the respiratory characteristic, and at least one physiological sensor disposed proximate to the subject and configured to detect a physiological characteristic of the subject, wherein the sensor subsystem is configured to generate and transmit at least one physiological signal representing the physiological characteristic, and a processor subsystem in communication with the sensor subsystem, the processor subsystem being configured to receive at least one of the at least one respiratory signal and the at least one physiological signal.

**13 Claims, 11 Drawing Sheets**



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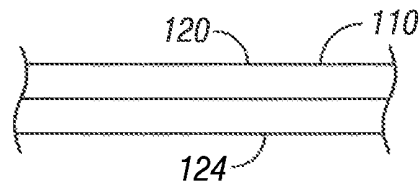


FIG. 14

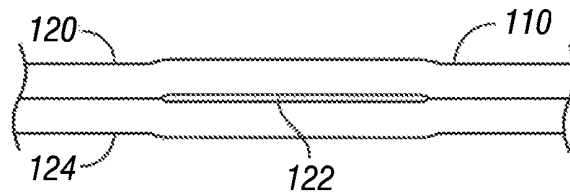


FIG. 15

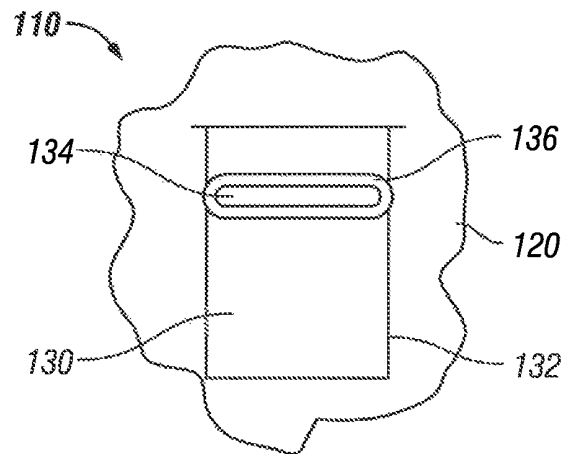


FIG. 16

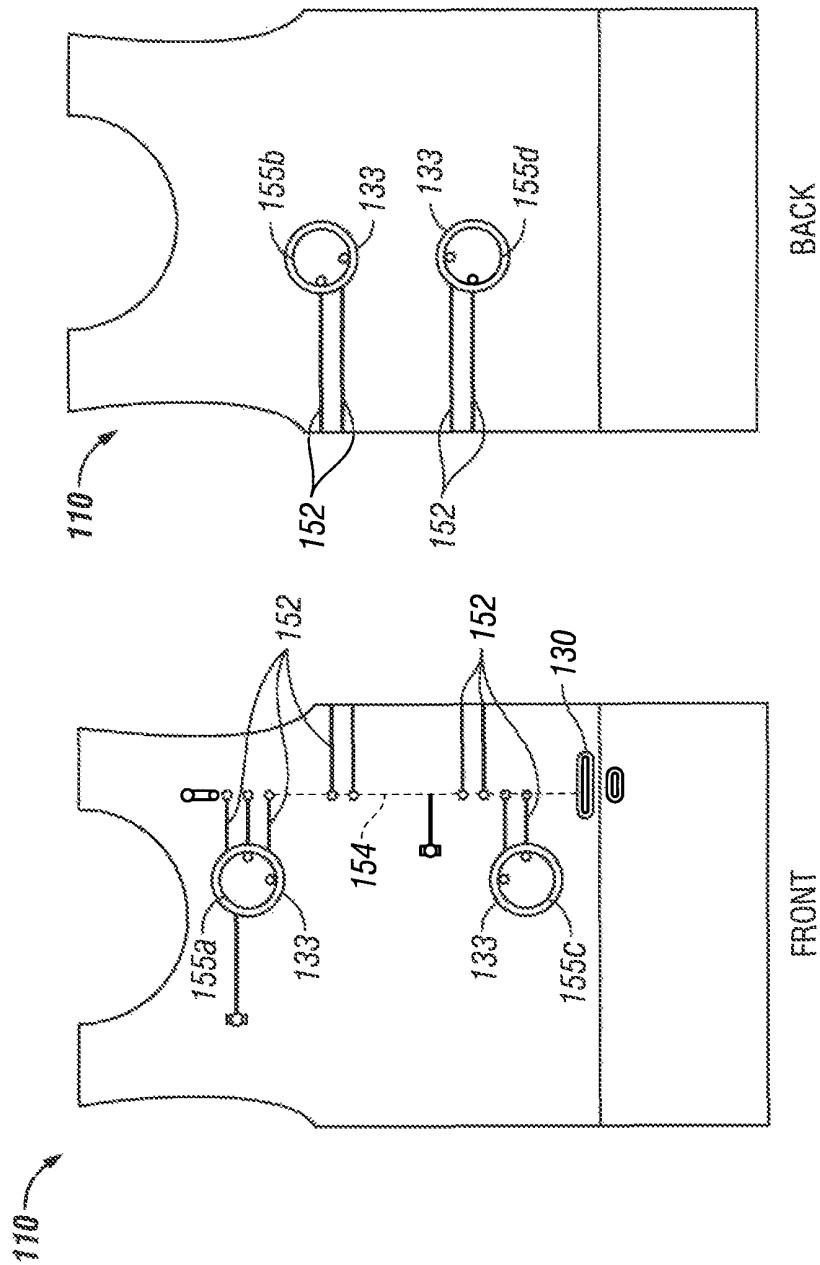


FIG. 18

FIG. 17

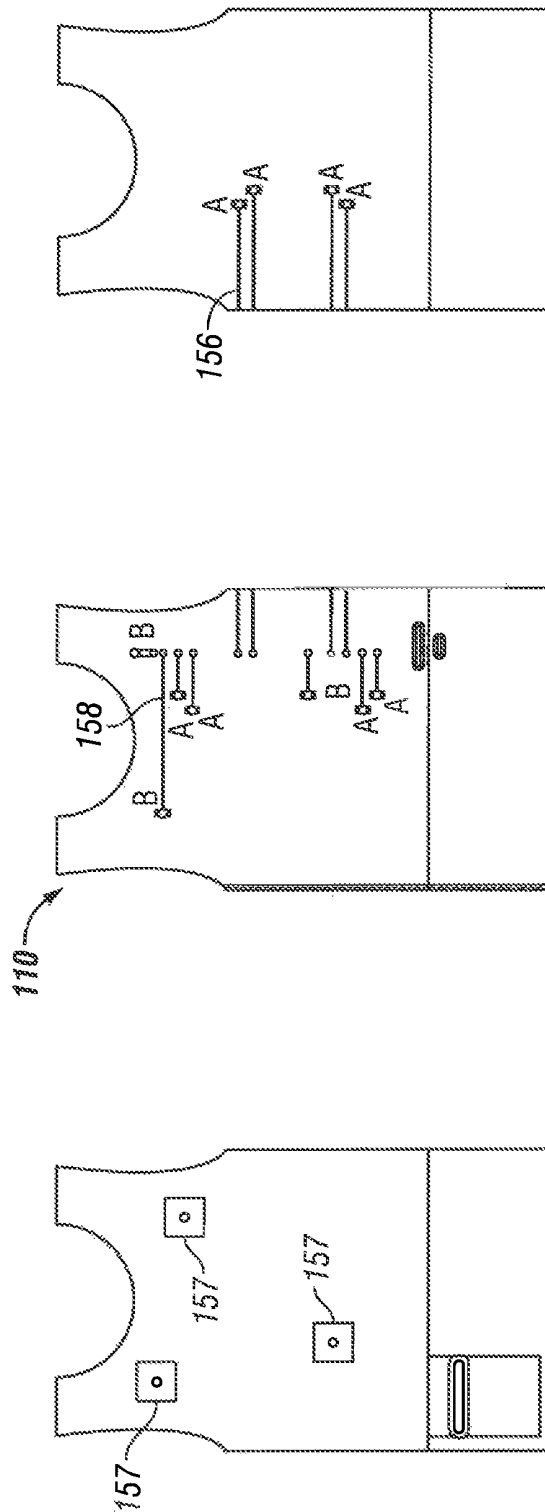


FIG. 21

FIG. 20

FIG. 19

**PHYSIOLOGICAL MONITORING GARMENT****CROSS-REFERENCE TO RELATED APPLICATIONS**

This non-provisional application claims priority to U.S. Provisional Application No. 61/275,633, filed Sep. 1, 2009, and is a continuation application of U.S. patent application Ser. No. 12/869,627, filed Aug. 26, 2010, now abandoned each of which is incorporated herein by reference in its entirety.

**FIELD OF THE INVENTION**

The present invention relates generally to methods and systems for monitoring physiological and athletic performance characteristics of a subject. More particularly, the invention relates to physiological and athletic performance monitoring garments and associated systems.

**BACKGROUND OF THE INVENTION**

In medical diagnosis and treatment of ambulatory and non-ambulatory subjects, it is often necessary and/or desirable to monitor one or more physiological and/or athletic performance characteristics and/or parameters associated with the subject. It has also often been desirable to monitor physiological characteristics of ambulatory subjects during potentially stressful or hazardous situations, such as those often encountered by first responders (e.g., firefighters, police, emergency medical personnel, etc.) and during athletic and/or competition training.

Various systems and methods have thus been developed to monitor physiological characteristics and parameters of ambulatory and non-ambulatory subjects. Earlier physiological monitoring systems typically included electrical or electronic components (e.g., a heart rate sensor) that were fastened to wearable items or placed in pouches in the items. Individual wires between the components were then fastened to the outside of the items or disposed partially or wholly in seams and the like. Illustrative is the harness system (used in military applications) disclosed in U.S. Pat. No. 6,198,394, issued Mar. 6, 2001, which is incorporated by reference herein in its entirety.

A major problem with the earlier wearable monitoring systems or items is that the wires were wholly or partially separate from the textile material, particularly at key connection regions. As a result, the wires could, and often did, catch on or become entangled with objects, and disconnect from components.

To overcome the noted problems with the earlier systems, wearable monitoring garments having electronic circuits and data transmission lines integrated in the textile material were developed. Illustrative are the wearable monitoring garments disclosed in U.S. Pat. No. 6,080,690, issued Jun. 27, 2000, U.S. Pat. No. 5,906,004, issued May 25, 1999, U.S. Pat. No. 6,727,197, issued Apr. 27, 2004, and U.S. patent application Ser. No. 10/922,336 (Publication No. 2005/0054941 A1), filed Aug. 20, 2004, each of which is incorporated by reference herein in its entirety.

In U.S. Pat. No. 6,080,690 and U.S. Pat. No. 5,906,004, wearable monitoring garments having conductive fibers are disclosed. The noted patents provide that the conductive fibers can be disposed in a multitude of positions and orientations within the garment to facilitate connection by and between one or more sensors and a controller.

A major drawback of the disclosed garments and systems is, however, that routing of data and power between components is limited without extensive formation of electrical and data junctions in the fabric. As is well known in the art, formation of such junctions often requires a very complex and expensive manufacturing process or processes.

In U.S. Pat. No. 6,727,197 and U.S. patent application Ser. No. 10/922,336, further wearable monitoring garments are disclosed. The monitoring garments similarly include conductive fibers to facilitate connection by and between components. The disclosed garments also include integrated (and in some instances "elongate stretchable") busses for providing power to components (e.g., sensors) and for routing component signals to signal transmission or processing circuitry.

Although the disclosed garments provide an effective integrated means for routing power and data between components, there are still several drawbacks and disadvantages associated with the disclosed garments (and systems). A major drawback is that the component connections remain complex and, hence, time consuming and expensive to manufacture.

It would therefore be desirable to provide an improved physiological monitoring garment that facilitates accurate, real-time determination of a plurality of physiological characteristics and is simple to manufacture.

**BRIEF SUMMARY OF THE INVENTION**

In accordance with the above objects and those that will be mentioned and will become apparent below, the present invention is directed to a wearable physiological and performance monitoring garment that facilitates monitoring of physiological and performance characteristics and parameters of a subject. In a preferred embodiment of the invention, the physiological monitoring garment includes integral component connecting and data transmission means that facilitates communication by and between components employed with the garment.

In some embodiments of the invention, the physiological monitoring garment includes a magnetometer system, which is embedded in or carried by the wearable garment. In some embodiments, the physiological monitoring garment includes additional physiological sensors, such as, for example, ECG, temperature, and blood oxygen sensors, and processing and monitoring means, which similarly are embedded in or carried by the wearable monitoring garment.

**BRIEF DESCRIPTION OF THE FIGURES**

Further features and advantages will become apparent from the following and more particular description of the present invention, as illustrated in the accompanying drawings, in which like referenced characters generally refer to the same parts or elements throughout the views.

FIG. 1 is a block diagram of a physiological monitoring system, according to one embodiment of the invention.

FIG. 2 is a schematic illustration of a magnetometer system, according to one embodiment of the invention.

FIG. 3 is a top plan view of a magnetometer, according to one embodiment of the invention.

FIG. 4 is a side plan view of the magnetometer shown in FIG. 3, according to one embodiment of the invention.

FIG. 5 is a schematic illustration of a magnetometer driver circuit, according to one embodiment of the invention.

FIG. 6 is a schematic illustration of a magnetometer preamplifier circuit, according to one embodiment of the invention,

FIG. 7 is a schematic illustration of a magnetometer input buffer amplifier circuit, according to one embodiment of the invention.

FIG. 8 is a side view of a subject, showing a position of the magnetometer system shown in FIG. 2 on the subject, according to one embodiment of the invention.

FIG. 9 is a perspective view of the subject showing the position of magnetometers on the front of the subject, according to one embodiment of the invention.

FIG. 10 is a plane view of the subject's back, showing the position of magnetometers thereon, according to one embodiment of the invention.

FIG. 11 is a front plan view of a physiological monitoring garment, according to one embodiment of the invention.

FIG. 12 is a front plan view of the physiological monitoring garment shown in

FIG. 11, showing a side opening thereof, according to one embodiment of the invention.

FIG. 13 is a front perspective view of a subject wearing the physiological monitoring garment shown in FIGS. 11 and 12, according to one embodiment of the invention.

FIG. 14 is a partial side, sectional view of a physiological monitoring garment, showing the top and bottom layers thereof, according to one embodiment of the invention.

FIG. 15 is a partial side, sectional view of a physiological monitoring garment, showing a pocket formed between the top and bottom layers thereof, according to one embodiment of the invention.

FIG. 16 is a front plan view of a pre-formed garment pocket, according to one embodiment of the invention.

FIG. 17 is a front plan view of a physiological monitoring garment having a plurality of integral garment conductors associated therewith, according to one embodiment of the invention.

FIG. 18 is a back plan view of the physiological monitoring garment shown in FIG. 17, according to one embodiment of the invention.

FIG. 19 is a back plan view of a physiological monitoring garment showing incorporated ECG sensor connections, according to one embodiment of the invention.

FIG. 20 is a front plan view of the physiological monitoring garment shown in FIG. 19 showing ECG and magnetometer circuits, according to one embodiment of the invention.

FIG. 21 is a back plan view of the physiological monitoring garment shown in FIG. 19 showing magnetometer circuits, according to one embodiment of the invention.

#### DETAILED DESCRIPTION OF THE INVENTION

Before describing the present invention in detail, it is to be understood that this invention is not limited to particularly exemplified garments, apparatuses, systems, circuits, or methods, as such may, of course, vary. Thus, although a number of wearable items, apparatuses, systems, and circuits similar or equivalent to those described herein can be used in the practice of the present invention, the preferred wearable items, apparatuses, systems, and circuits are described herein.

It is also to be understood that the terminology used herein is for the purpose of describing particular embodiments of the invention only and is not intended to be limiting.

Unless defined otherwise, all technical and scientific terms used herein have the same meaning as commonly understood by one having ordinary skill in the art to which the invention pertains.

As used in this specification and the appended claims, the singular forms "a", "an", and "the" include plural referents unless the content clearly dictates otherwise.

Further, all publications, patents, and patent applications referenced herein, whether supra or infra, are hereby incorporated by reference in their entirety.

The publications discussed herein are provided solely for their disclosure prior to the filing date of the present application. Nothing herein is to be construed as an admission that the present invention is not entitled to antedate such publication(s) by virtue of prior invention. Further, the dates of publication may be different from the actual publication dates, which may need to be independently confirmed.

#### Definitions

The terms "respiratory parameter" and "respiratory characteristic", as used herein, mean and include a characteristic associated with the respiratory system and functioning thereof, including, without limitation, breathing frequency (f<sub>B</sub>), tidal volume (V<sub>T</sub>), inspiration volume (V<sub>I</sub>), expiration volume (V<sub>E</sub>), minute ventilation (VE), inspiratory breathing time, expiratory breathing time, and flow rates (e.g., rates of change in the chest wall volume). The terms "respiratory parameter" and "respiratory characteristic" further mean and include inferences regarding ventilatory mechanics from synchronous or asynchronous movements of the chest wall compartments.

According to the present invention, flow rates and respiratory accelerations can be determined from a volume signal. Further, numerous inferences regarding ventilatory mechanics can be drawn from the degree of asynchrony in movement occurring among the discrete compartments that make up the chest wall.

The terms "physiological parameter" and "physiological characteristic", as used herein, mean and include, without limitation, electrical activity of the heart, electrical activity of other muscles, electrical activity of the brain, pulse rate, blood pressure, blood oxygen saturation level, skin temperature, and core temperature.

The terms "spatial parameter" and "spatial characteristic", as used herein, mean and include a subject's orientation and/or movement.

The term "garment", as used herein, means and includes any item that is adapted to cover at least a portion of a subject's body, including, without limitation, a shirt, vest, jacket, band, and the like.

The terms "patient" and "subject", as used herein, mean and include humans and animals.

Pulmonary ventilation, tidal volume, respiratory rate, and other associated respiratory characteristics can provide a reliable and practical measure of oxygen and carbon dioxide transpiration in a living body. Respiratory characteristics are directly connected to exercise effort, physiological stress, and other physiological characteristics. One way to externally determine tidal volume is to measure the change in thoracic volume. Change in thoracic volume is caused by the expansion and contraction of the lungs. As the gas pressure in the lungs at the maxima and minima of the pressure ranges is equilibrated to surrounding air pressure, there is a very close and monotonic relationship between the volume of the lungs and the volume of air inspired.

Accurate measurement of the change in thoracic volume involves measuring the change in the diameter of the chest at the ribcage. Measurement of the change in the diameter of the chest below the ribcage can provide additional accuracy to the measurement. Monitoring changes in the diameter of the chest below the ribcage can account for diaphragm delivered breathing where the contraction and relaxation of the diaphragm muscle causes the organs of the abdomen to be pushed down and outwards, thereby increasing the available volume of the lungs.

Monitoring and analyzing respiratory characteristics can be particularly useful in athletic applications, as there is a direct link between performance and an athlete's processing of oxygen and carbon dioxide. For example, in many athletic training situations, it is helpful to know when the athlete's body transitions between aerobic exercise and anaerobic exercise, sometimes referred to as the athlete's ventilatory threshold. Crossing over the ventilatory threshold level is an indicator of pending performance limitations during sport activities. For example, it can be beneficial for athletes to train in the anaerobic state for limited periods of time. However, for many sports, proper training requires only limited periods of anaerobic exercise interrupted by lower intensity aerobic exercises. It is difficult for an athlete to determine which state, anaerobic or aerobic, he or she is in without referencing physiological characteristics such as respiratory characteristics. Therefore, respiratory monitoring and data processing can provide substantial benefits in athletic training by allowing for accurate and substantially instantaneous measurements of the athlete's exercise state. Changes in an athlete's ventilatory threshold over time, as well as patterns of tidal volume during post-exercise recovery, can be valuable to measure improvements in the athlete's fitness level over the course of a training regime. Respiratory monitoring can further allow for monitoring and analyzing changes in a subject's resting metabolic rate.

A second ventilatory threshold exists at the point when the load on the body is such that the pulmonary ventilation is no longer sufficient to support life sustainably. Dwelling too long in this state will lead to collapse and so determination of this point can be of value in medical applications, and particularly to first responders and other emergency response personnel.

The present invention is directed to a wearable physiological monitoring garment that facilitates monitoring of physiological and performance characteristics and parameters of a subject. As indicated above, the physiological monitoring garment includes integral component connecting and data transmission means that facilitates communication by and between components employed with the garment.

In some embodiments of the invention, the physiological monitoring garment includes a magnetometer system, which is embedded in or carried by the wearable garment. As discussed in detail below, the magnetometer system facilitates accurate real-time determination of various respiratory characteristics and parameters.

In some embodiments, the physiological monitoring garment includes additional physiological sensors and processing and monitoring means, which similarly are embedded in or carried by the wearable monitoring garment. The physiological sensors can include, without limitation, sensors that are adapted to monitor and record electrical activity of the brain, heart, and other muscles (e.g., EEG, ECG, EMG), pulse rate, blood oxygen saturation level (e.g., SpO<sub>2</sub>), skin temperature, and core temperature. Physiological parameters measured and/or calculated may include, for example, heart rate, respiration rate, blood oxygen level, blood flow, hydration status, calories burned, muscle fatigue, and/or body temperature.

As will readily be appreciated by one having ordinary skill in the art, the wearable physiological monitoring garment of the invention facilitates accurate, real-time determination of a plurality of respiratory and other physiological parameters and characteristics. The monitoring garment also readily accommodates ambulatory home and outpatient monitoring, and monitoring subjects during potentially stressful or hazardous situations and athletic and/or competition training.

Several embodiments of the wearable physiological monitoring garment and associated systems of the invention will now be described in detail. It is, however, to be understood that the invention is not limited to the garment(s) and systems described herein. Indeed, as will be appreciated by one having ordinary skill in the art, garments and systems similar or equivalent to the described garment and systems can also be employed within the scope of the present invention.

**Physiological Monitoring System**

Referring first to FIG. 1, there is shown a block diagram of an exemplary physiological monitoring system **10** that can be employed with the physiological monitoring garment of the invention. As discussed in detail below, in one embodiment of the invention, the physiological monitoring system **10** is adapted to (i) monitor and detect changes in (or displacements of) the anteroposterior diameters of the rib cage and abdomen, and axial displacement of the chest wall, and (ii) determine anatomical, physiological, and performance information associated with the monitored subject as a function of the magnetometer signals reflecting the noted anatomical displacements.

As illustrated in FIG. 1, the physiology monitoring system **10** preferably includes a data acquisition subsystem **20**, a control-data processing subsystem **40**, a data transmission subsystem **50**, a data monitoring subsystem **60**, and a power source **70**, such as a battery.

In one embodiment of the invention, the data acquisition subsystem **20** includes a magnetometer system **21** having paired magnetometers that are adapted to monitor and detect changes in (or displacements of) the anteroposterior diameters of a subject's rib cage and abdomen, and axial displacement of the subject's chest wall when the magnetometers are disposed at selective anatomical subject positions. It is, however, understood that the invention is not limited to the use of paired magnetometers to measure displacements of a subject's rib cage, abdomen, and chest wall.

Although the present invention is described herein in terms of magnetometers and magnetometer systems, it is understood that other types of sensor systems capable of measuring changes in distance between two or more sensors in the system can be used in place of, or in addition to, magnetometers. Specifically, the invention is not limited to the use of electromagnetic coils or magnetometers to acquire signals representing measured changes in the anteroposterior diameters of the rib cage and abdomen, and axial displacement of the chest wall. Various additional means and devices that can be readily adapted to measure the noted anatomical parameters can be employed within the scope of the invention. Such means and devices include, without limitation, Hall effect sensors and electronic compass sensors. Wireless sensors with the capability of measuring time delay in a signal sent from one sensor to another and thereby determine the distance between the two sensors can be substituted for or provided in addition to magnetometers in accordance with the present invention.

Magnetometers (or other sensors) can be embedded in or carried by a wearable garment, such as a shirt or vest. The wearable monitoring garment eliminates the need to attach the magnetometers directly to the skin of a subject and, hence, resolves all issues related thereto. The wearable monitoring garment also facilitates repeated and convenient positioning of magnetometers at virtually any appropriate (or desired) position on a subject's torso.

According to the invention, at least one, and preferably two, magnetometers are employed to measure the noted subject parameters (or displacements). In some embodiments of

the invention, two pairs of magnetometers are thus employed. In some embodiments, more than two pairs of magnetometers are employed.

Referring to FIG. 2, in one embodiment of the invention, magnetometer system 21 includes first transmission magnetometer 22a, first receive magnetometers 22b, second transmission magnetometer 24a, and second receive magnetometers 24b. The paired magnetometers 22a, 22b and 24a, 24b being responsive to changes in spaced distances therebetween. As discussed in detail below, first transmission magnetometer 22a is adapted to transmit a first electromagnetic field and first receive magnetometer 22b is adapted to receive the first electromagnetic field. First receive magnetometer 22b is responsive to changes in the first electromagnetic field (and, hence, the spaced distance between paired magnetometers 22a, 22b) and further adapted to generate and transmit a first signal representing a first change in the first electromagnetic field. The electromagnetic coils of embodiments of the present invention are described as “receiving” or “transmitting,” however, each receiving coil can alternatively and independently be a transmitting coil, and each transmitting coil can alternatively and independently be a receiving coil. Coils can also perform both receiving and transmitting functions.

Second transmission magnetometer 24a is adapted to transmit a second electromagnetic field and second receive magnetometer 24b is adapted to receive the second electromagnetic field. In one embodiment, second receive magnetometer 24b is responsive to changes in the first and second electromagnetic fields (and, hence, the spaced distances between paired magnetometers 24a, 24b and magnetometers 22a, 24b) and is further adapted to transmit a second signal representing a first change in the second electromagnetic field and a third signal representing a second change in the first electromagnetic field.

Referring now to FIGS. 3-7, the novel magnetometers of the invention will be described in detail. It is, however, understood that the invention is not limited to the magnetometer embodiments described herein. Indeed, as will be appreciated by one having ordinary skill in the art, various conventional magnetometers can be readily employed within the scope of the invention to monitor and/or measure anatomical distances or parameters.

Referring first to FIGS. 3 and 4, there is shown one embodiment of a low profile magnetometer 80 of the invention. In one embodiment of the invention, the magnetometer 80 comprises a multi-layer printed circuit having a conductive circular coil 72.

According to the invention, conductive coil 72 can be formed by winding the coil using standard conducting wires, such as copper, aluminum or other conductive metals, or they can be fabricated using standard multi-layer printed circuit techniques. In one embodiment, the coil is formed from 6-layer printed circuit boards with 18 turns on each layer, approximately 2 inches in diameter, with layers connected together in series using standard printed circuit layer connectors (“vias”) to form a 108 turn coil.

It is understood that different sized coils can be formed in the same fashion or by winding on a thin form and adhering the coils to a flexible substrate. This coil form factor differs from previous respiratory magnetometer designs which utilize a solenoid design—a long thin coil formed around a ferromagnetic rod.

The magnetometer 80 (and associated system) preferably operates over a physical range of 10 cm to 40 cm laterally and 20 cm to 50 cm axially with the ability to measure displacement over those distances very accurately. The system noise

is also extremely low, less than 10 nV/rtHz, which translates into a measurement error of 50 microns rms.

In one embodiment, power is supplied to the magnetometer 80 via a battery with a voltage range of approximately 2.8 V to 3.7 V.

Since the magnetometer circuitry is connected to coils that will be in an uncontrolled environment, all connections are preferably balanced over a very wide frequency range. Balancing all external connections minimizes electromagnetic compatibility (EMC) effects, both radiation and susceptibility, and ensure the system is extremely robust in the presence of electrostatic discharge (ESD) events. Balanced connections will also add 60 dB+reduction in rejecting AC mains parasitic pickup.

Preferably, the circuit is divided into smaller circuit blocks. The blocks can include (i) a microcontroller, (ii) analog-to-digital converter (ADC), storage, and digital signal processing (DSP), (iii) drivers, (iv) preamplifiers, and (v) input buffers. Each of the circuit blocks are discussed in detail below.

According to the invention, the driver circuitry converts square wave drive from the microcontroller into efficient current drive for each coil and provides monitoring of the actual drive signals back to the microcontroller (see FIG. 5). The op-amps provide buffering of the microcontroller’s outputs and isolation from the coils back to the microcontroller.

Since many microcontrollers have adequate current drive capability, buffering may not be required (depending on the selection of the microcontroller).

The impedance matching network of capacitors is used to match the relatively high voltage drive of the square wave to the low voltage drive requirement of the coil. This takes advantage of the Q in the circuit, enhances the fundamental frequency component of the drive, and provides isolation to the coils. Using this technique, the coils are driven with approximately 5.8 mA using only 1 mA from the power supply.

The protection diodes provide clamping to known voltages during ESD events.

Each diode has less than 1 pF capacitance. The diodes will thus not affect the normal circuit operation.

According to the invention, the preamplifier circuit provides a matching network to the coil with low-noise gain to retrieve the small signals from the coil (see FIG. 6).

In the illustrated embodiment, the preamp includes a simple two NPN transistor structure. This topology takes advantage of the low-power 2N5088 high-beta transistor to provide gain of approximately 90 at the carrier frequency. The bypass capacitors are selected to provide rejection of the mains frequency (50/60 Hz) of over 90:1. The output of the preamp is offset from ground by Vbe.

The output follower is designed and adapted to lower the output impedance of the preamp without increasing the power consumption. The voltage drop Vbe across 100 kΩ requires only 6 uA of power supply current, yet lowers the output impedance to less than 120 Ω.

Preferably, the preamp has an input noise density function of 10 nV/VHz and consumes approximately 14 uA.

The capacitor network provides matching the low impedance of the coil to the relatively high impedance of the preamp, which adds an additional gain of 4. The total gain of the preamplifier is thus 360.

According to the invention, the input buffer amplifier provides additional gain of 25, amplifying the signal enough to be digitized by the microcontroller (see FIG. 7). Since the signals from the preamp are in the range of 0.5 mV to 60 mV, it is unlikely that this stage will saturate. Op-amps may be

employed since the signals would be large enough at this point to cause unacceptable distortion if simple transistor amplifiers were used.

According to the invention, various families of effective microcontroller chips can be employed within the scope of the invention. In one embodiment a TI MSF430, manufactured by Texas Instruments, microcontroller chip is employed. The noted chip is small in area and requires less than 3.5 mA of current.

The requirements of the DSP function is to provide four square waves to the drivers; one pair preferably at 8.95 kHz and the other pair preferably at 8.85 kHz. Each pair of square waves is 180 degrees out of phase.

Preferably, the microcontroller has the capability to provide 12 bit digitization of 8 channels at a rate of more than 20 kHz. Being differential, the input values are preferably processed in pairs.

In one embodiment, the eight channels are reduced to 4 values, representing TxA, TxB, Rx1, and Rx2 at each sample in time.

At the same sampling rate, four products are preferably created: TxA\*Rx1, TxA\*Rx2, TxB\*Rx1, and TxB\*Rx2. These four products are accumulated into four registers for a run length of Ss/Sps. The run length, or packet size, is therefore 400.

Preferably, every 400 accumulations the four values are retrieved, calibration factors adjust their values, and the respiration sample values are supplied to the main controller.

Referring back to FIG. 1, according to the invention, control-data processing subsystem 40 includes programs, instructions, and associated algorithms to control data acquisition subsystem 20 (and, hence, magnetometers associated therewith), data transmission subsystem 50, and monitoring subsystem 60.

Control-data processing subsystem 40 is further programmed and adapted to retrieve and process magnetometer signals reflecting changes in the magnetometer fields (and, hence, changes in spaced distances between the paired magnetometers) and to determine anatomical, physiological, and/or performance information associated with the monitored subject (as a function of the magnetometer signals), including at least one respiratory characteristic (more preferably, a plurality of respiratory characteristics). Control-data processing subsystem 40 is also referred to herein as "processor subsystem," "processing subsystem," and "data processing subsystem." The terms control-data processing subsystem, processor subsystem, processing subsystem, and data processing subsystem are used interchangeably in the present application.

Data monitoring subsystem 60 is designed and adapted to display physiological and performance characteristics and parameters generated and transmitted by control-data processing subsystem 40.

According to embodiments of the invention, data transmission subsystem 50 is programmed and adapted to monitor and control the noted communication links and, hence, transmissions by and between data acquisition subsystem 20, control-data processing subsystem 40, and data monitoring subsystem 60.

Further details of the noted physiological monitoring system are set forth in U.S. Provisional Application No. 61/275,575, filed Sep. 1, 2009, and co-pending U.S. application Ser. No. 12/869,582, filed Aug. 26, 2010, each of which is incorporated by reference herein in its entirety.

As will be readily appreciated by one having ordinary skill in the art, the magnetometers of the invention can be disposed in various anatomically appropriate positions on a subject to

monitor and measure the change in distance (or displacement) between the magnetometers. Referring now to FIGS. 8-10, there is shown paired magnetometers 22a, 22b, 24a, 24b positioned on a subject or patient 100, in accordance with the inventions disclosed in the above referenced U.S. Provisional Application No. 61/275,575, U.S. application Ser. No. 12/869,582, and co-Pending U.S. application Ser. No. 12/231,692, which is similarly incorporated by reference herein in its entirety.

As illustrated in FIGS. 8-10, the first transmission magnetometer (i.e., first transmitter) 22a is preferably positioned on front 101 of subject 100 proximate the umbilicus of subject 100, and the first receive magnetometer (i.e., first receiver) 22b is preferably positioned proximate the same axial position, but on back 102 of the subject 100. Second receive magnetometer (i.e., second receiver) 24b is preferably positioned on front 101 of subject 100 proximate the base of the sternum and second transmission magnetometer (i.e. second transmitter) 24a is positioned proximate the same axial position, but on back 102 of subject 100.

As subject or patient 100 breathes, displacement(s) of the rib cage and abdomen (i.e., changes in the distance between each pair of coils 22a, 22b and 24a, 24b, denoted, respectively, by arrow 29 and arrow 25), is determined from measured changes in voltage between paired coils 22a, 22b and 24a, 24b. The axial displacement of the chest wall, denoted by arrow 23, (e.g., xiphi-umbilical distance (Xi)), is also determined from measured changes in voltage between transmission coil 22a and receive coil 24b. In this embodiment magnetometer 24b is a dual-function electromagnetic coil, where "dual function coil" refers to a coil capable of receiving transmissions from a plurality of different transmission coils (i.e., magnetometer 24b is adapted to receive magnetic field transmissions from magnetometers 22a and 24a).

As indicated above, the measured displacements are typically employed to determine anatomical and physiological information associated with the monitored subject 100, including at least one respiratory characteristic. As set forth in U.S. Provisional Application No. 61/275,575, filed Sep. 1, 2009, and co-pending U.S. application Ser. No. 12/869,582, additional paired magnetometers can also be employed, and the multiple measured displacements can be employed to assess additional anatomical, physiological, and performance characteristics, such as determining and characterizing the relationship(s) of chest wall movement(s) to respiratory activity and respiratory associated events such as speaking, sneezing, laughing, and coughing.

As also set forth in U.S. Provisional Application No. 61/275,575, filed Sep. 1, 2009, and co-pending U.S. application Ser. No. 12/869,582, data acquisition subsystem 20 can additionally include at least one additional physiological sensor (preferably, a plurality of additional physiological sensors) adapted to monitor and record one or more physiological characteristics associated with monitored subject 100. The physiological sensors can include, without limitation, sensors that are adapted to monitor and record electrical activity of the brain, heart, and other muscles (e.g., EEG, ECG, EMG), pulse rate, blood oxygen saturation level (e.g., SpO<sub>2</sub>), skin temperature, and core temperature. Physiological parameters measured and/or calculated may include, for example, heart rate, respiration rate, blood oxygen level, blood flow, hydration status, calories burned, muscle fatigue, and/or body temperature.

Exemplary physiological sensors (and associated systems) are disclosed in U.S. Pat. No. 6,551,252, issued Apr. 22, 2003, U.S. Pat. No. 7,267,652, issued Sep. 11, 2007, co-pending U.S. patent application Ser. No. 11/764,527, filed Jun. 18,

2007, and International Application No. PCT/US2005/021433, each of which is incorporated by reference herein in its entirety.

Data acquisition subsystem **20** can also include one or more audio sensors, such as, for example, a microphone, for monitoring sounds generated by a monitored subject, and a speaker to enable two-way communication by and between the monitored subject and a monitoring station or individual.

In some embodiments of the invention, the data acquisition subsystem **20** can include means for directly monitoring the subject's orientation and/or movement, e.g., spatial parameters. According to the invention, various conventional means can be employed to monitor or measure subject orientation and movement, including optical encoders, proximity and Hall effect switches, laser interferometry, accelerometers, gyroscopes, and/or global positioning systems (GPS).

In one embodiment, the means for directly monitoring the orientation and movement of a subject includes at least one multi-function inertial sensor (e.g., 3-axis accelerometer or 3-axis gyroscope). As is well known in the art, orientation and motion of a subject can be readily determined from the signals or data transmitted by a multi-function inertial sensor.

#### Physiological Monitoring Garment

As indicated above, the physiological monitoring garment of the invention includes a wearable garment that is configured and adapted to cooperate with the aforementioned physiological monitoring system. The physiological monitoring garment can thus include paired magnetometers, such as paired magnetometers **22a**, **22b**, **24a**, **24b**, discussed above and/or one or more physiological sensors and associated processors, control units and circuits. The physiological sensors can include, without limitation, sensors that are adapted to monitor and record electrical activity of the brain, heart, and other muscles (e.g., EEG, ECG, EMG), pulse rate, blood oxygen saturation level (e.g., SpO<sub>2</sub>), skin temperature, and core temperature. Physiological parameters measured and/or calculated may include, for example, heart rate, respiration rate, blood oxygen level, blood flow, hydration status, calories burned, muscle fatigue, and/or body temperature.

According to the invention, the physiological monitoring garment can include various garments or items that are adapted to cover at least a portion of a subject's body, such as a shirt, vest, jacket, band, and the like. It is thus to be understood that, although the monitoring garment describe below includes a vest, the invention is not limited to the described garment.

Referring now to FIGS. **11-13**, there is shown one embodiment of a physiological monitoring garment **110** of the invention. As illustrated in FIG. **13**, the monitoring garment **110** preferably includes a body conforming garment (in this instance, a body conforming sleeveless shirt or vest).

The physiological monitoring garment or vest **110** preferably includes a front panel or section **112** and a rear panel or section **114**, having an opening **111** that is preferably disposed on one side of vest **110**. In the illustrated embodiment, vest **110** further includes a bottom panel or section **116**.

As illustrated in FIG. **12**, front panel **112** and rear panel **114** include cooperating closure means **115a** that secures vest **110** to the subject's torso. According to the invention, various conventional closure means, such as a hook and pile system, e.g., VELCRO® such as that manufactured by Velcro, Inc., snaps, a zipper, etc., can be incorporated into vest **110** to facilitate closure thereof.

In a preferred embodiment of the invention, closure means **115a** includes an integral conventional zipper system. In one embodiment, the zipper system closure means **115a** is adapted and positioned to close front panel **112** and rear panel

**114** and to secure vest **110** to a subject's body by moving a zipper tab **115b** and, hence, engaging the zipper teeth in a downward direction (denoted by Arrow A).

According to the invention, vest **110** can include any material that is suitable for a wearable garment or clothing. In one embodiment, vest **110** includes an elastic material, e.g., a polyurethane-polyurea copolymer such as LYCRA® material made by DuPont, that allows vest **110** to conform to the body shape (i.e. body conforming) when secured thereon.

Referring now to FIGS. **14** and **15**, in one embodiment vest **110** includes outer layer **120** and inner layer **124**, each layer **120**, **124** preferably including the same material. Disposed at appropriate anatomical and/or desired positions on vest **100** is at least one garment pocket **122** (preferably a plurality of garment pockets **122**).

According to the invention, the pockets **122** can include various shapes and sizes to facilitate receipt and secure positioning of selective monitoring system components, (e.g., magnetometers **22a**, **22b**, **24a**, **24b**, physiological sensors, and associated processors control units, etc.).

Pockets **122** can also be formed by various conventional means. In one embodiment, pockets **122** are formed by cutting an opening in one panel (e.g., panel **120** or **124**) and forming a closed pocket with the desired size and shape by sewing the border thereof. In one embodiment, pre-formed pockets are sewn on or within vest **110** (e.g., between vest panels **120**, **124**).

Referring now to FIG. **16**, there is shown one embodiment of a pre-formed pocket **130** of the invention. Pocket **130** includes an opening **134** that is disposed, in this instance, proximate the top of pocket **130**. In a preferred embodiment, opening **134** is reinforced.

In the illustrated embodiment, pocket **130** is sewn (denoted generally with reference character "132") between vest panels **120**, **124**. As indicated above, pocket **130** can also be sewn to or on the outer surface of top panel **120** or bottom panel **124**.

As indicated above, pockets **122**, **130** are configured and adapted to receive and securely position selective monitoring system **10** components, such as, for example, employed magnetometers, processors, control units, etc.

As also indicated above, the magnetometers (e.g., magnetometers **22a**, **22b**, **24a**, **24b**), and additional sensors, if employed, can be positioned on or in vest **110** at virtually any desired position, whereby, when vest **110** is worn by a subject the magnetometers and other sensors are positioned proximate any anatomically appropriate or desired position on the subject's body.

To facilitate power transmission to and communication by and between the monitoring system components, vest **110** further includes at least one garment circuit (preferably a plurality of garment circuits) having at least one integral garment conductor associated therewith.

Referring now to FIGS. **17** and **18**, there is shown an embodiment of the physiological monitoring garment **110** having a plurality of integral garment conductors associated therewith. As illustrated in FIGS. **17** and **18**, in some embodiments of the invention, the garment **110** includes a first plurality of integral conductors or pathways **152**. In some embodiments, the first plurality of integral conductors **152** are substantially horizontally disposed. In some embodiments, the first plurality of integral conductors comprise stretchable conductors.

According to the invention, the various electrically conductive materials can be incorporated into garment **110** by, for example, weaving, knitting, or surface application to provide (or construct) the first plurality of integral conductors **152**

and, hence, to facilitate connection by and between sensors, such as the magnetometers, and an electronic unit.

According to the invention, the incorporation of these conducting pathways **152** are chosen based on the fabric assembly technique (e.g., knitted or woven). Potential embodiments include silver plated or silver containing threads, and other conductive thread materials, with the exclusion of traditional copper wiring.

In some embodiments of the invention, the garment **110** includes at least one conductive connector (more preferably a plurality of conductive connectors) that facilitates connection by and between sensors and related components disposed on the outer garment layer **120** and the inner garment layer **124**. In one embodiment, the connectors include silver plated snap fasteners.

According to the invention, the physiological monitoring garment **110** also includes a central communications pathway (shown in phantom and designated generally with the reference character “**154**”) in communication with the first plurality of integral conductors **152**. According to the invention, the central communications pathway **154** can include a ribbon containing fine wires, a series of discrete channels containing strips of metalized or otherwise electrically conductive yarns, thread, or fabric.

In the illustrated embodiment shown in FIGS. **17** and **18**, the monitoring system **10** associated with the physiological monitoring garment **110** includes a magnetometer system, (e.g., paired magnetometers **155a**, **155b**, **155c**, **155d**, and at least one ECG sensor, not shown). As illustrated in FIGS. **17** and **18**, monitoring garment **110** thus includes pockets **133** configured to receive and securely position the paired magnetometers **155a**, **155b**, **155c**, **155d**.

Referring to FIGS. **19-21**, the physiological monitoring garment **110** further includes associated magnetometer circuit **156** and ECG circuit **158**. In one embodiment of the invention, magnetometer circuit **156** includes pairs of conductors that are vertically oriented along one side of the shirt and connected to horizontal conductors woven into garment **110**. According to the invention, connection between the vertical pairs and horizontal pairs can be effected by stitching with conductive materials, connecting with conductive epoxy, or preferably by standard miniature garment snap fasteners attached to the vertical conductors and to the horizontal conductors by standard crimped-on piercing fasteners.

In one embodiment, similar pairs of vertical and horizontal conductors are employed for magnetometers positioned over the thorax and abdomen area of garment **110**.

In one embodiment of the invention, the ECG circuit **158** includes pairs of conductors that are vertically oriented along one side of the shirt and connected to horizontal conductors woven into garment **110**. Connection between the vertical pairs and horizontal pairs can similarly be effected by stitching with conductive materials, connecting with conductive epoxy, or preferably by standard miniature garment snap fasteners attached to the vertical conductors and to the horizontal conductors by standard crimped-on piercing fasteners.

Further, in some embodiments, the horizontal conductors are terminated in woven-in conductive patches **157** located proximal to the desired locations for sensing the electrical activity of the heart. The patches **157** can serve directly as the ECG sensors or can be electrically connected to standard adhesive ECG electrodes by, for example, the inclusion of crimped-on snap fasteners within the patches.

#### Garment Construction

Construction of the monitoring garment of the invention will now be described in detail. It is however to be understood the construction described below is merely one exemplary

method of constructing the monitoring garment and is not meant to limit the scope of the invention in any manner.

In one embodiment, garment **110** is constructed by a semi-automated process, wherein a tubular garment section is knitted using conductive and non-conductive threads. The garment section includes horizontal conductive areas knitted into what will become the outer layer of garment **110**, conductive patches knitted into the areas that will be ECG electrodes in the inner layer of the garment **110**, a separate elastically knitted band that will form the waist-band of garment **110**, and a pocket to receive the electronics module.

In a separate operation, a woven ribbon connector is fabricated from metallic conductive threads and non-conductive material. A crimped-on connector is attached to one end, and snap fasteners are attached vertically at break-out points for connection to the knitted horizontal conductors. The tube is folded over on itself to position the inner layer inside the outer layer, arm and neck openings are formed, and the waist-band is sewn on. Snap fasteners are attached to the garment, making connections to the ECG patches from the outside layer conductors, and providing connection points to the vertical ribbon cable.

Pockets for the magnetometers, ribbon cable, and electronics module are formed by processes, such as, for example, sonic welding, stitching, to adhesive. The magnetometers are attached using snap fasteners, and the vertical ribbon is inserted and connected to the knitted conductors by snap fasteners.

As will readily be appreciated by one having ordinary skill in the art, the physiological and performance monitoring garment and associated systems of the invention, described above, provide numerous significant advantages over conventional physiology monitoring methods and systems. Among the advantages is the provision of a physiological monitoring garment that provides accurate, real-time determination of a plurality of physiological characteristics, does not impede mobility, and is simple to manufacture. The physiological monitoring garment is also useful in numerous applications, including ambulatory home and outpatient monitoring, and monitoring subjects during potentially stressful or hazardous situations and athletic and/or competition training.

Additional advantages and applications of the present invention are apparent with reference to the systems and methods disclosed in U.S. patent application Ser. No. 12/869,578, filed Aug. 26, 2010, U.S. patent application Ser. No. 12/869,582, filed Aug. 26, 2010, U.S. patent application Ser. No. 12/869,576, filed Aug. 26, 2010, U.S. patent application Ser. No. 12/869,585, filed Aug. 26, 2010, U.S. patent application Ser. No. 12/869,592, filed Aug. 26, 2010, U.S. patent application Ser. No. 12/869,625, filed Aug. 26, 2010, and U.S. patent application Ser. No. 12/869,586, filed Aug. 26, 2010, each of which is incorporated by reference herein in its entirety.

Without departing from the spirit and scope of this invention, one of ordinary skill can make various changes and modifications to the invention to adapt it to various usages and conditions. As such, these changes and modifications are properly, equitably, and intended to be, within the full range of equivalence of the invention.

What is claimed is:

1. A fitness monitoring system for monitoring physiological parameters of a subject engaged in a physical activity, comprising:

a sensor subsystem including a first sensor and a second sensor, wherein the first sensor comprises a multi-layered printed circuit comprising a conductive circular coil formed from a plurality of printed circuit boards;

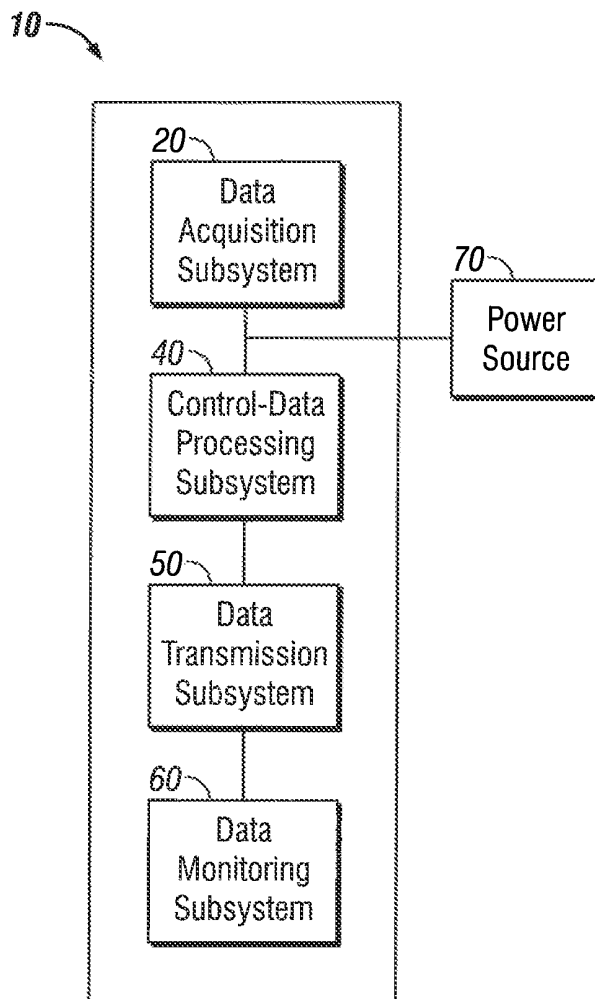


FIG. 1

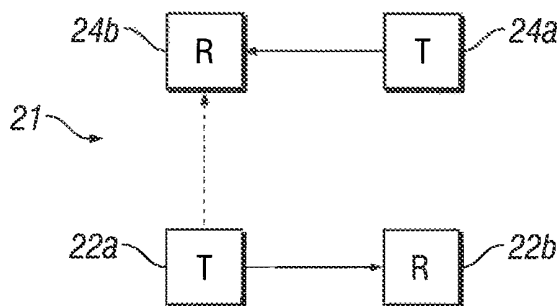


FIG. 2

a microcontroller; and  
 driver circuitry configured to convert a square wave drive  
 from the microcontroller into an efficient current drive  
 for the coil,  
 wherein each layer of the multi-layered printed circuit  
 comprises a continuous turn of the coil on one of the  
 printed circuit boards,  
 wherein the turns of the coil are connected in series,  
 wherein the first and second sensors are responsive to  
 changes in a parameter, and  
 wherein the sensor subsystem is configured to generate and  
 transmit a signal representative of the parameter.

2. The system of claim 1, wherein:  
 the conductive circular coil comprises a six-layer printed  
 circuit board having eighteen turns on each layer.

3. The system of claim 2, wherein the coil is approximately  
 two inches in diameter.

4. The system of claim 1, wherein the layers are connected  
 together in series using printed circuit layer connectors.

5. The system of claim 1, further comprising a battery with  
 a voltage range of approximately 2.8V to 3.7V, configured to  
 supply power to the sensor subsystem.

6. The system of claim 1,  
 wherein the driver circuitry is configured to provide moni-  
 toring of actual drive signals to the microcontroller.

7. The system of claim 1, further comprising:  
 a processor subsystem in communication with the sensor  
 subsystem and configured to receive the signal, wherein  
 the processor subsystem is programmed and adapted to  
 control the sensor subsystem and to process the signal,  
 and wherein the processor subsystem includes a rela-  
 tionship for determining a respiratory characteristic  
 from the signal, and wherein the processor subsystem is  
 adapted to generate and transmit a respiratory parameter  
 signal representing the respiratory parameter.

8. The system of claim 1, wherein the first and second  
 sensors are responsive to changes in the distance therebe-  
 tween, and wherein the signal represents a change in the  
 distance between the first and second sensors.

9. The system of claim 1, further comprising a capacitor  
 network configured to match the square wave drive to a volt-  
 age drive requirement of the coil.

10. The system of claim 1, wherein the sensor subsystem  
 includes a device for monitoring the subject's movement.

11. The system of claim 10, wherein the sensor subsystem  
 includes an inertial sensor.

12. The system of claim 10, wherein the sensor subsystem  
 includes a GPS receiver.

13. The system of claim 1, wherein the conductive circular  
 coil comprises a plurality of continuous turns on each layer of  
 the multi-layered printed circuit.

\* \* \* \* \*

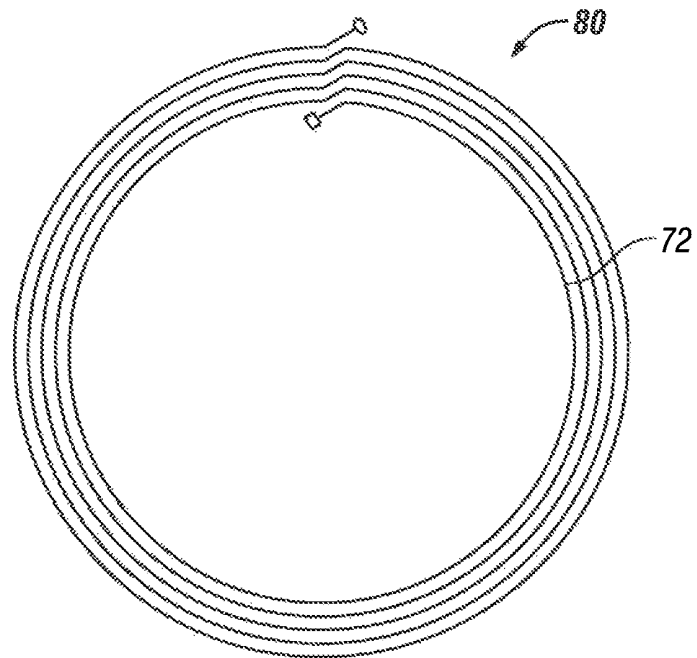


FIG. 3

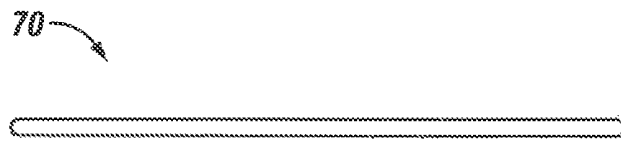


FIG. 4

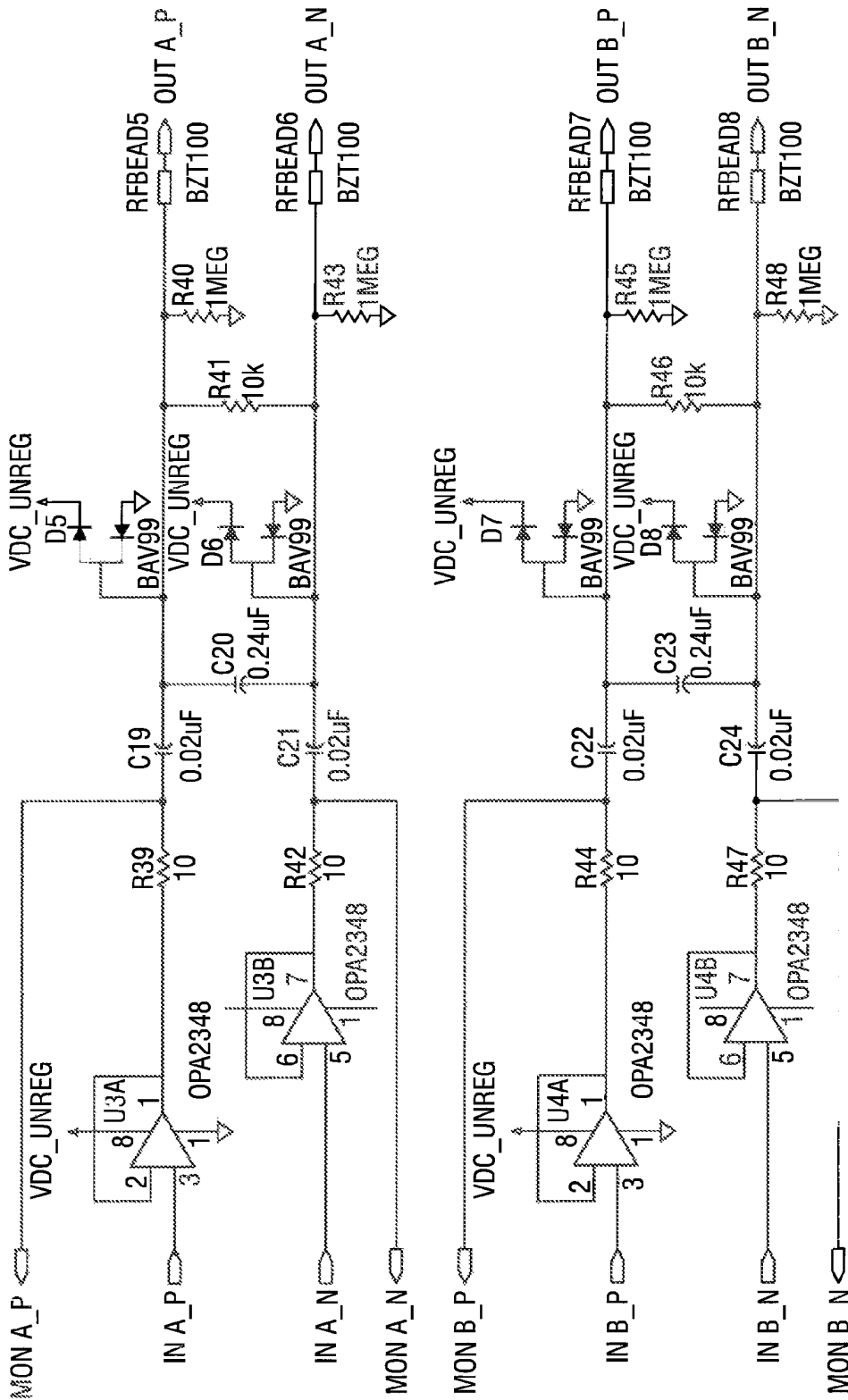


FIG. 5

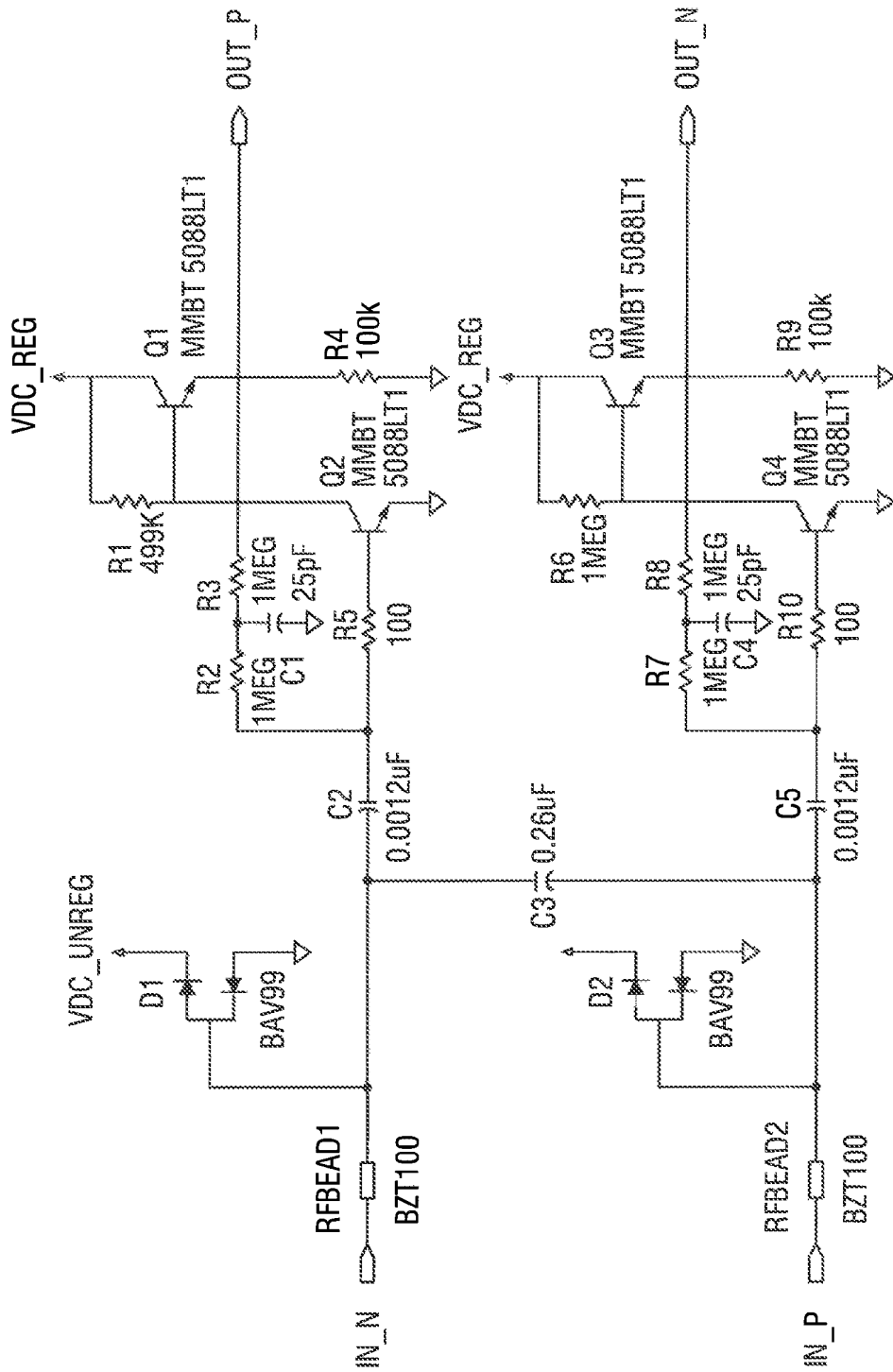


FIG. 6

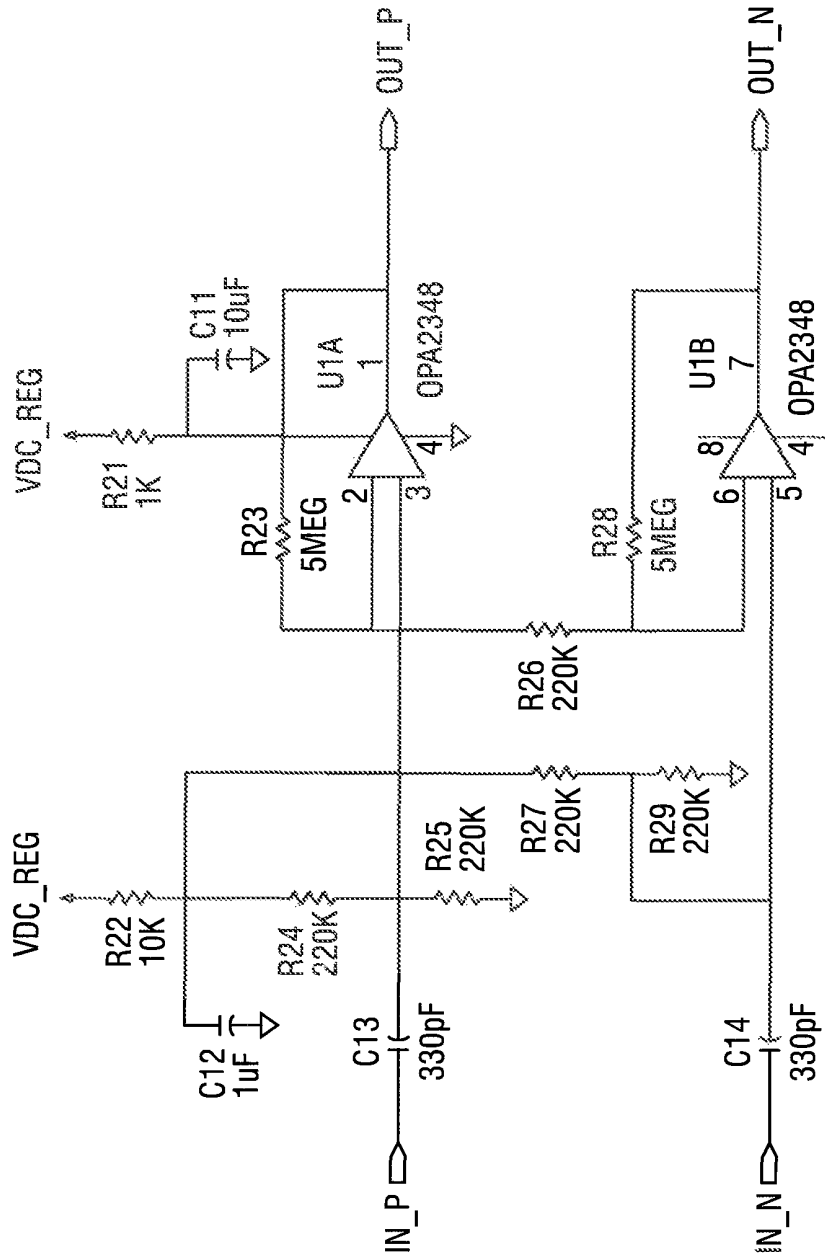


FIG. 7

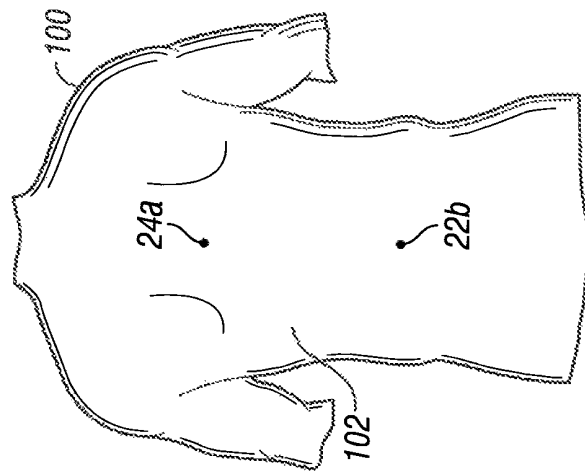


FIG. 10

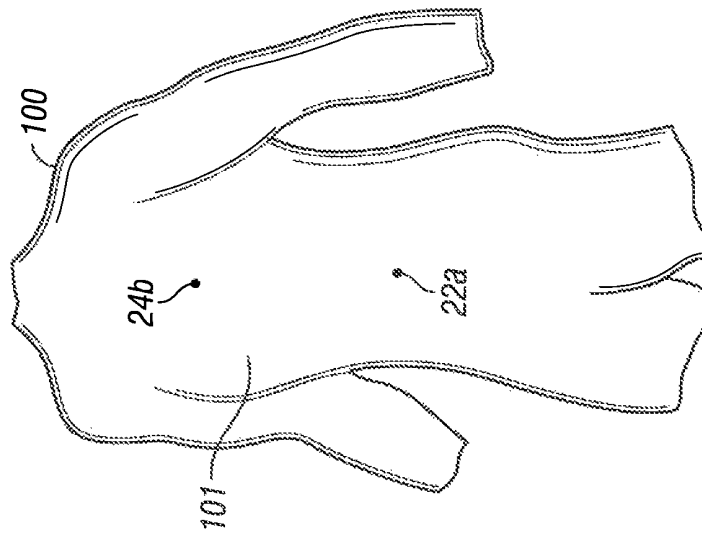


FIG. 9

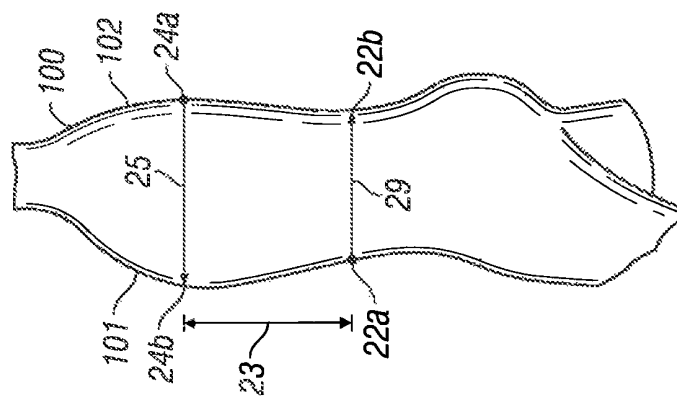


FIG. 8

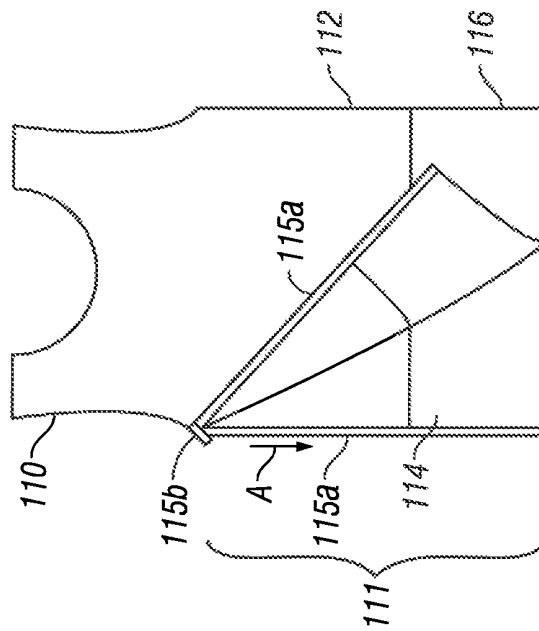


FIG. 11

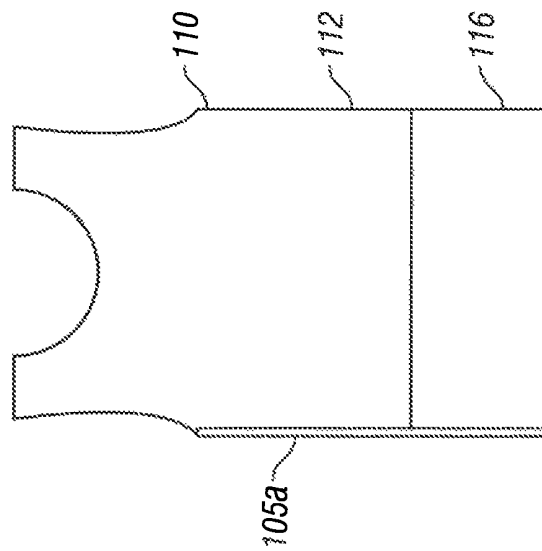
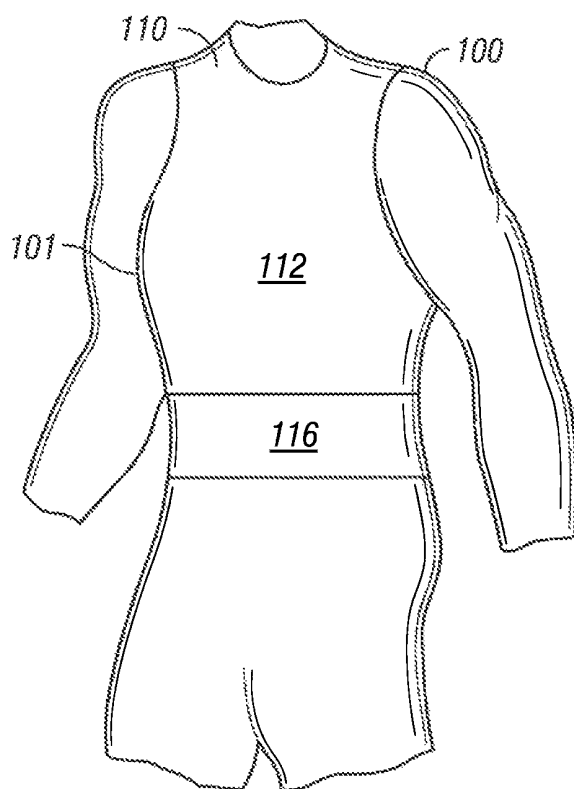


FIG. 12



**FIG. 13**

专利名称(译)	生理监测服装		
公开(公告)号	<a href="#">US8475371</a>	公开(公告)日	2013-07-02
申请号	US12/872174	申请日	2010-08-31
[标]申请(专利权)人(译)	阿迪达斯股份公司		
申请(专利权)人(译)	阿迪达斯世界体育		
当前申请(专利权)人(译)	阿迪达斯		
[标]发明人	DERCHAK P ALEXANDER CZAPLA LARRY ROGAN CATHERINE ANNE		
发明人	DERCHAK, P. ALEXANDER CZAPLA, LARRY ROGAN, CATHERINE ANNE		
IPC分类号	A61B5/00		
CPC分类号	A61B5/0816 A61B5/0823 A61B5/1135 A61B5/6805 A61B5/0488 A61B5/0476 A61B5/0402 A61B5/02055 A61B5/01 A61B5/0008 A61B5/0006 A61B5/14542 A61B5/0205 A61B2503/10 A61B2562/0223 G06F19/3418 Y10T442/109		
代理机构(译)	STERNE凯斯勒戈尔茨坦和FOX PLLC		
助理审查员(译)	ARCHER, MARIE		
优先权	61/275633 2009-09-01 US		
其他公开文献	US20110105861A1		
外部链接	<a href="#">Espacenet</a> <a href="#">USPTO</a>		

摘要(译)

本发明涉及用于监测受试者特征的系统和方法。根据本发明显例性实施例的系统包括传感器子系统，该传感器子系统包括至少一个呼吸传感器，该呼吸传感器设置在受试者附近并且被配置为检测受试者的呼吸特征，其中传感器子系统被配置为产生并传输至少一个呼吸表示呼吸特征的信号，以及至少一个生理传感器，其设置在受试者附近并且被配置为检测受试者的生理特征，其中传感器子系统被配置为生成并发送表示生理特征的至少一个生理信号，以及处理器子系统与传感器子系统通信，处理器子系统被配置为接收至少一个呼吸信号和至少一个生理信号中的至少一个。

