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(54) **METHODS AND APPARATUSES FOR LOCALIZING MYOCARDIAL INFARCTION DURING CATHETERIZATION**

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See application file for complete search history.

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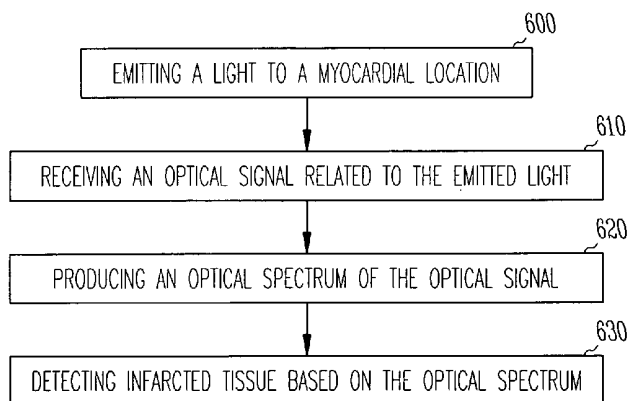
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(57) **ABSTRACT**

A catheter with a tissue property sensor provides for localization of myocardial infarction (MI) by utilizing one or more differences between properties of infarcted myocardial tissue and properties of normal myocardial tissue. The tissue property sensor is to be placed on endocardial wall or epicardial wall during catheterization to sense at least one tissue property allowing for detection of MI. Examples of the tissue property sensor include, but are not limited to, an optical sensor, an acoustic sensor, a contractility sensor, a temperature sensor, and a drug response sensor. In one embodiment, the tissue property sensor senses a tissue property in various locations on endocardial wall or epicardial wall and detects substantial changes in the tissue property that indicate a boundary between infarcted tissue and normal tissue.

23 Claims, 8 Drawing Sheets



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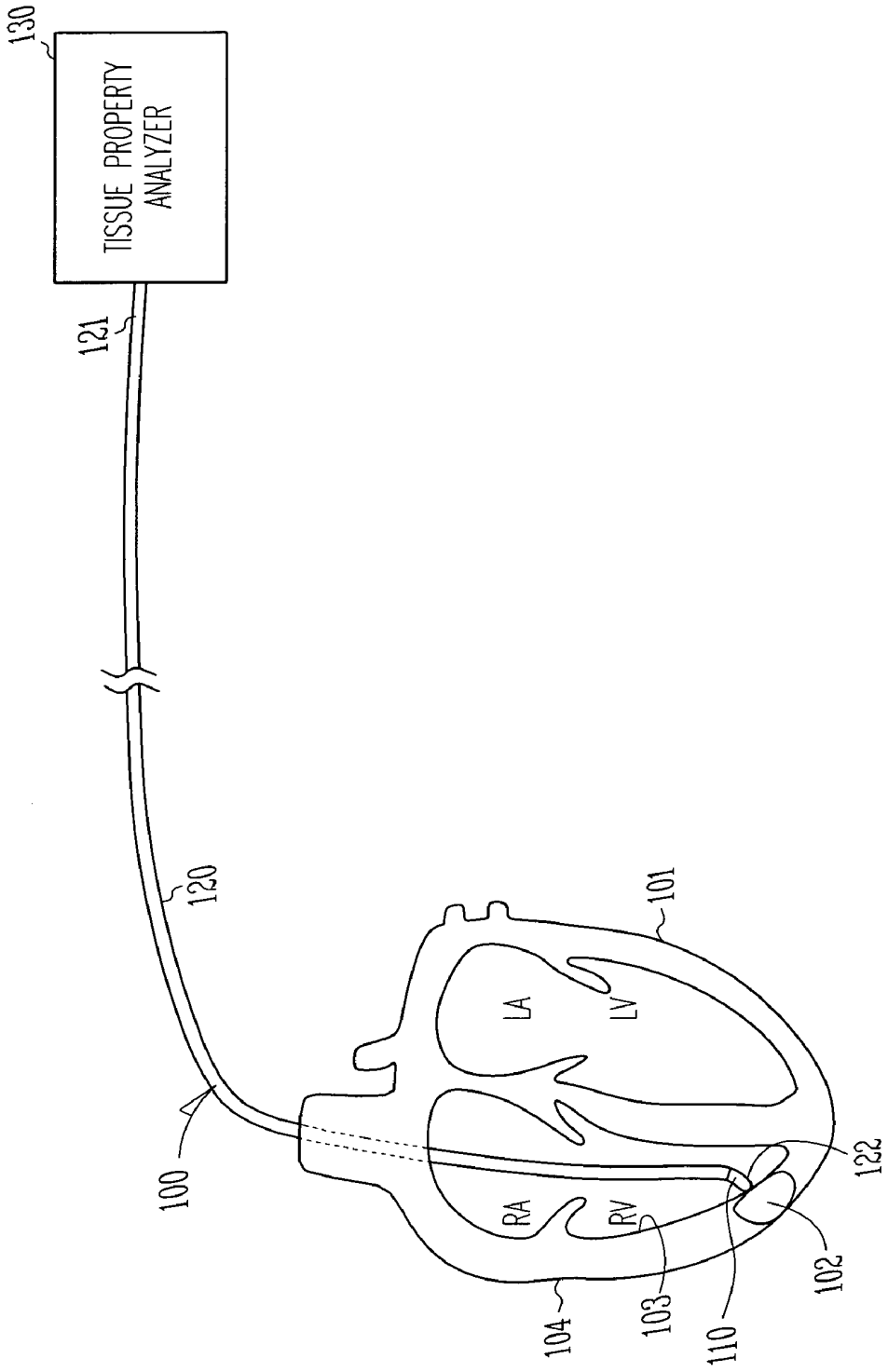


FIG. 1

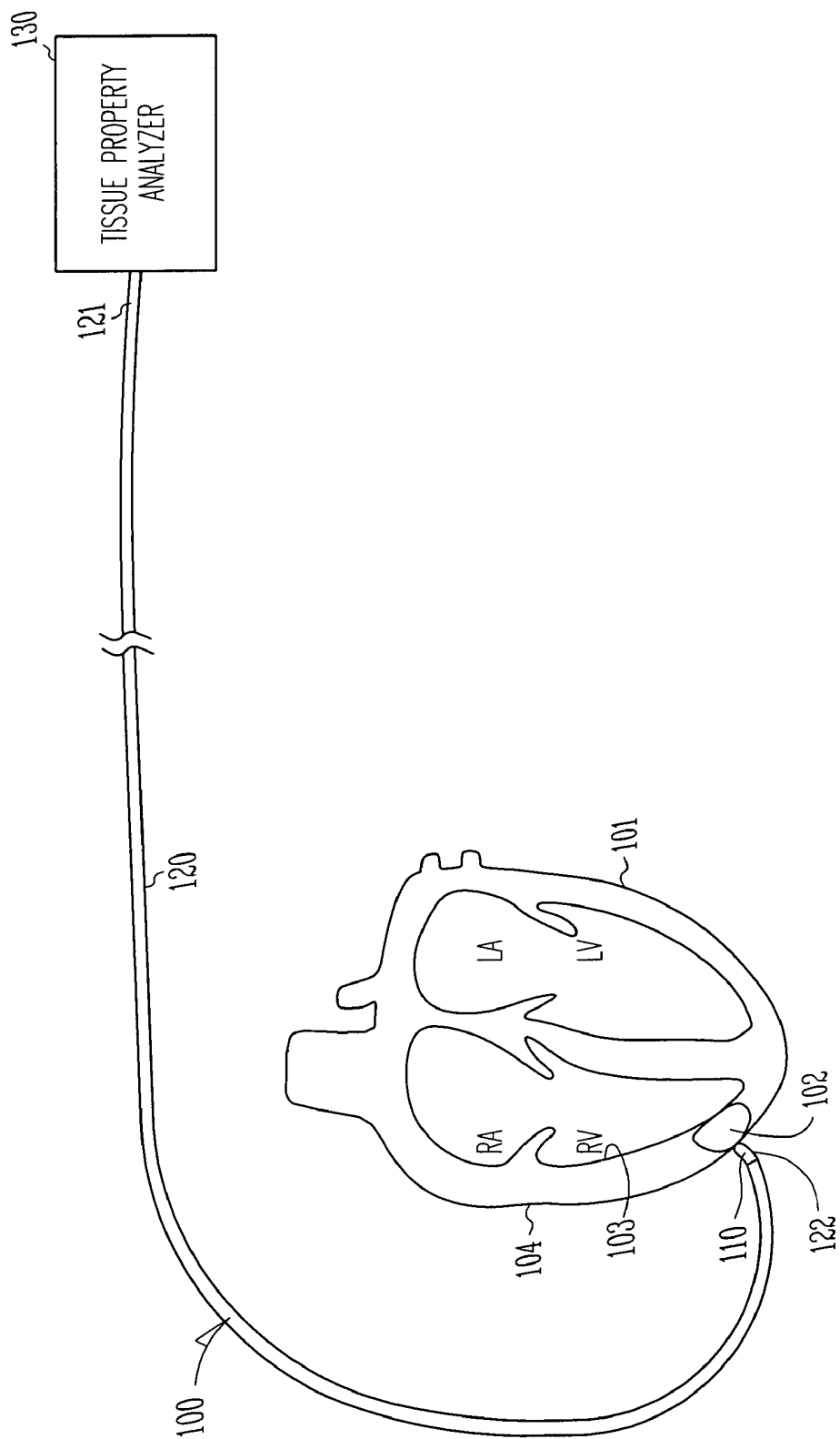


FIG. 2

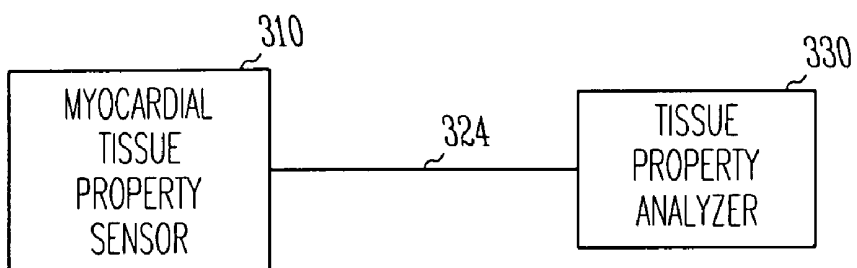


Fig.3

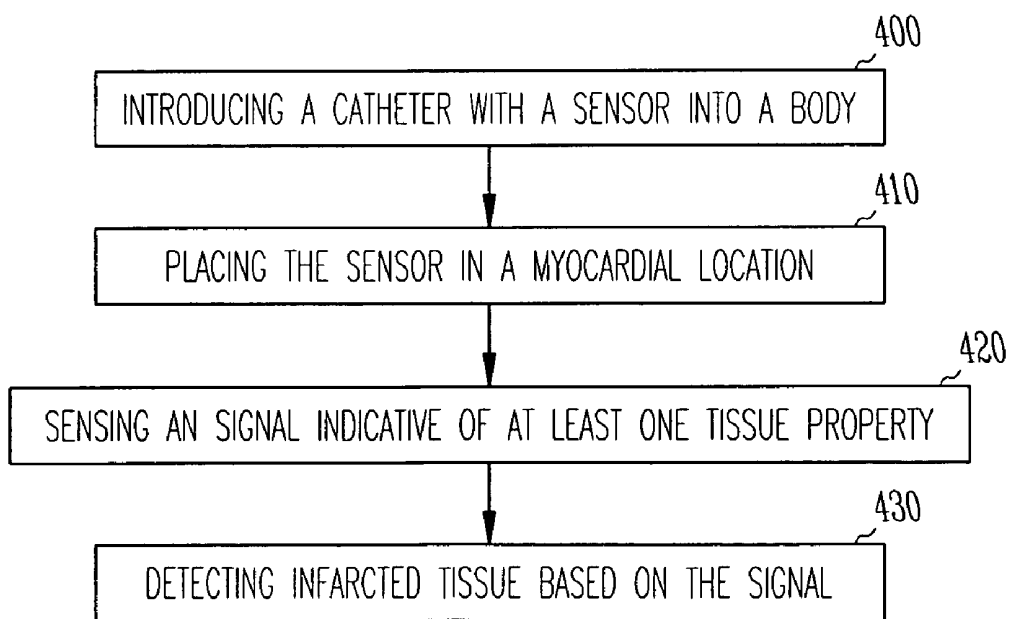


Fig.4

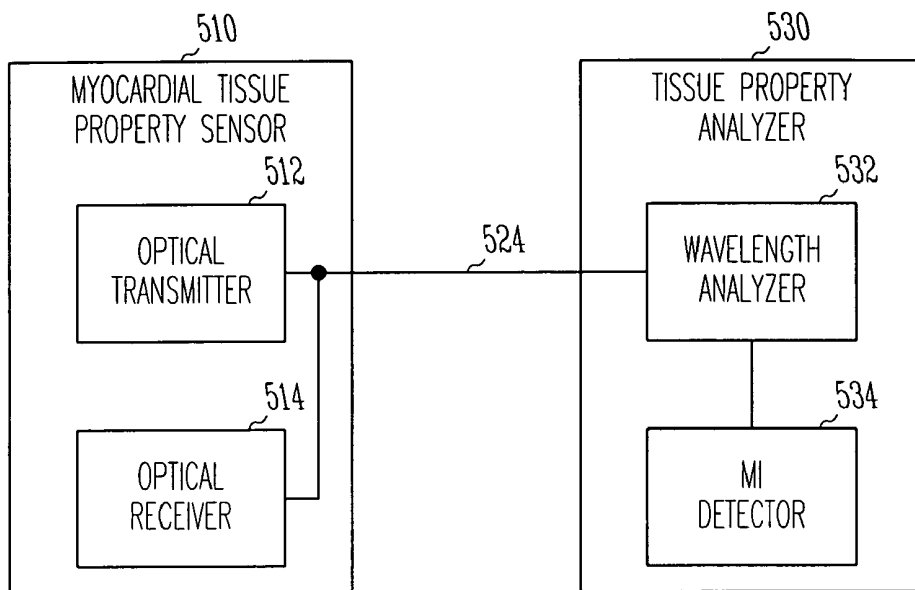


Fig.5

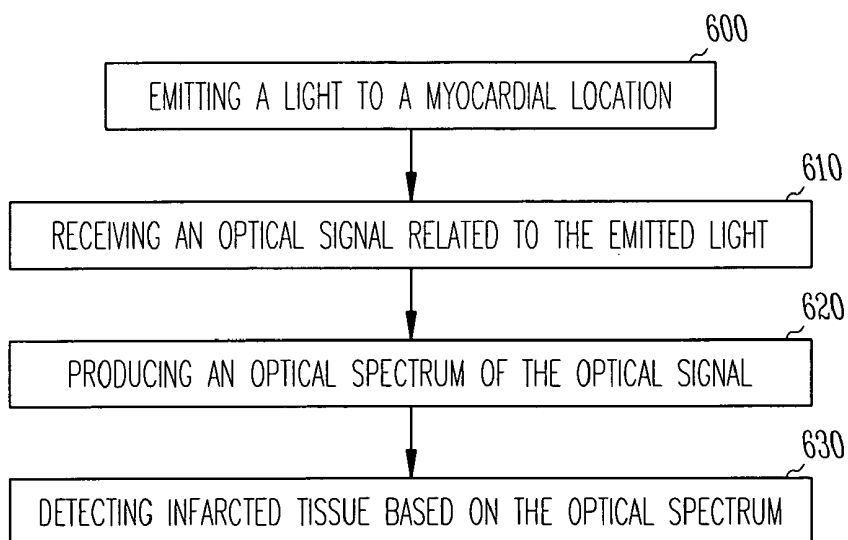


Fig.6

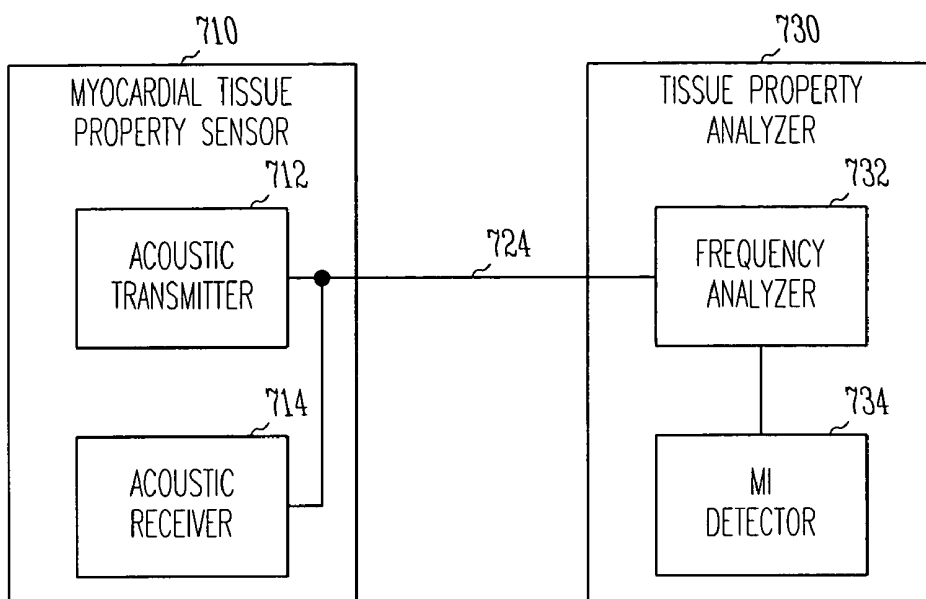


Fig.7

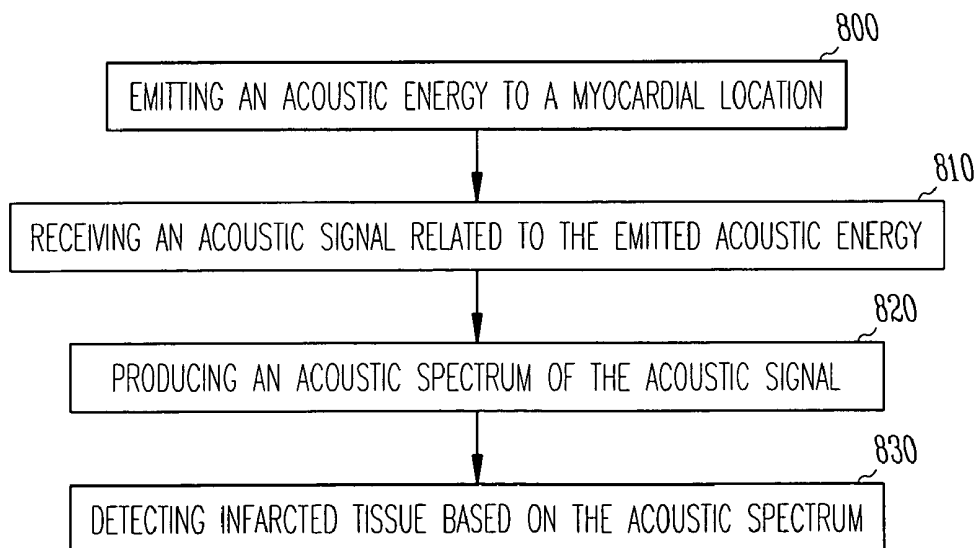


Fig.8

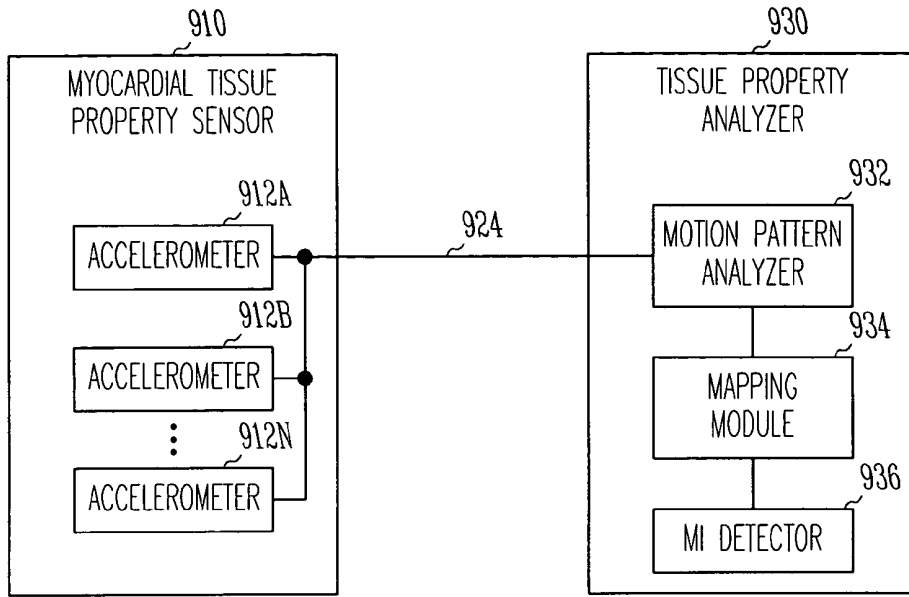


Fig.9

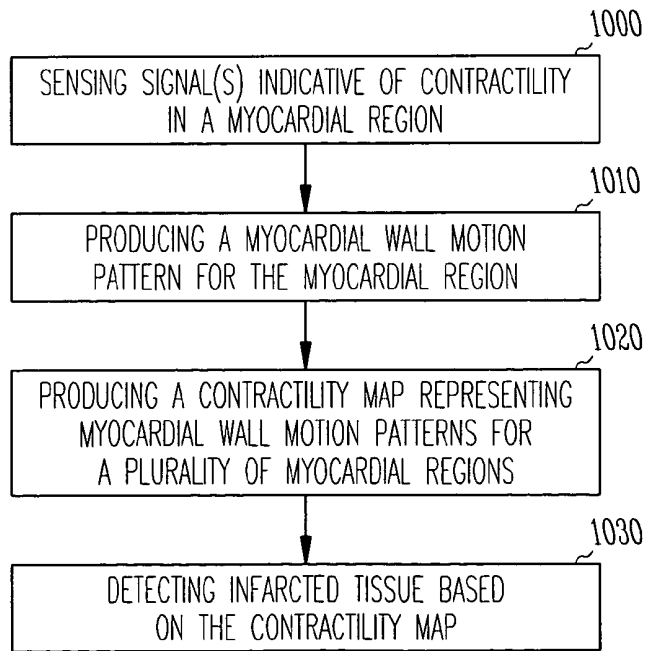


Fig.10

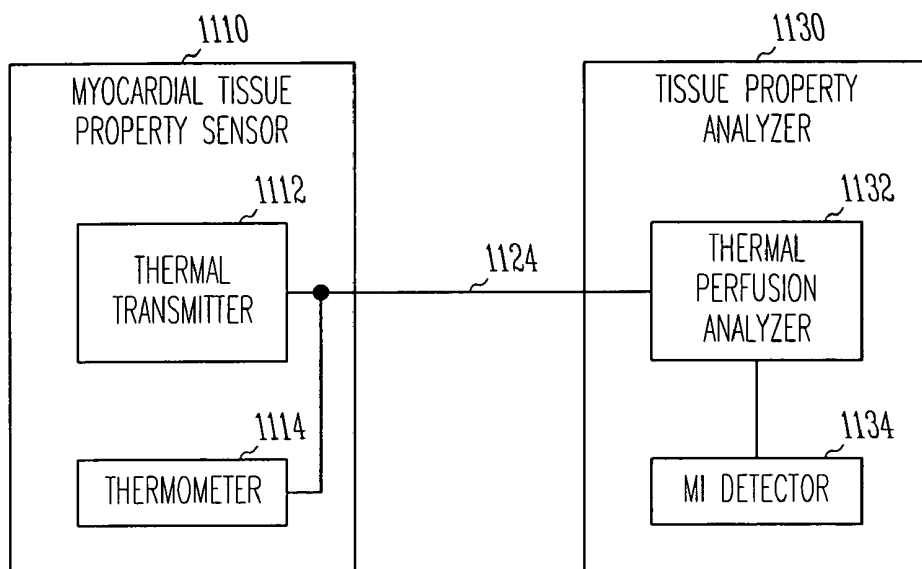


Fig.11

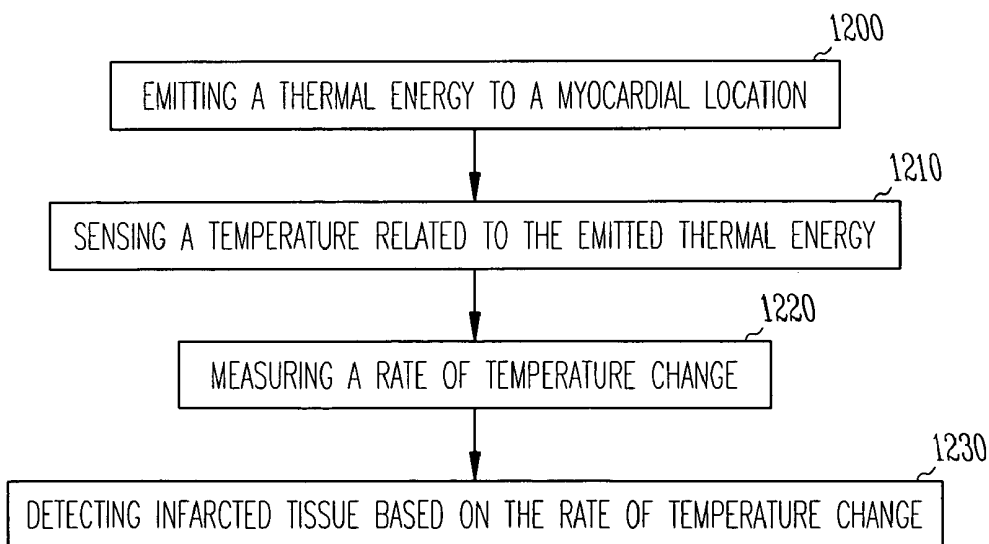


Fig.12

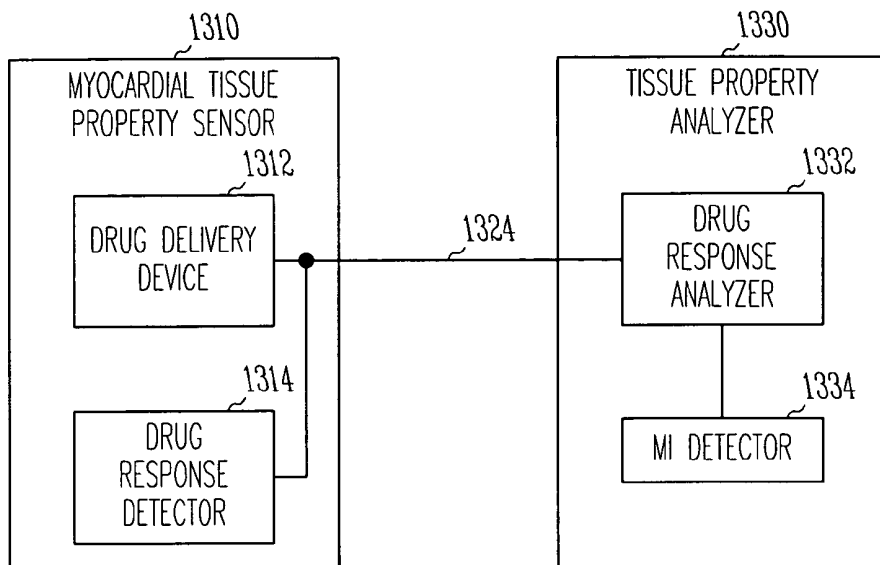


Fig.13

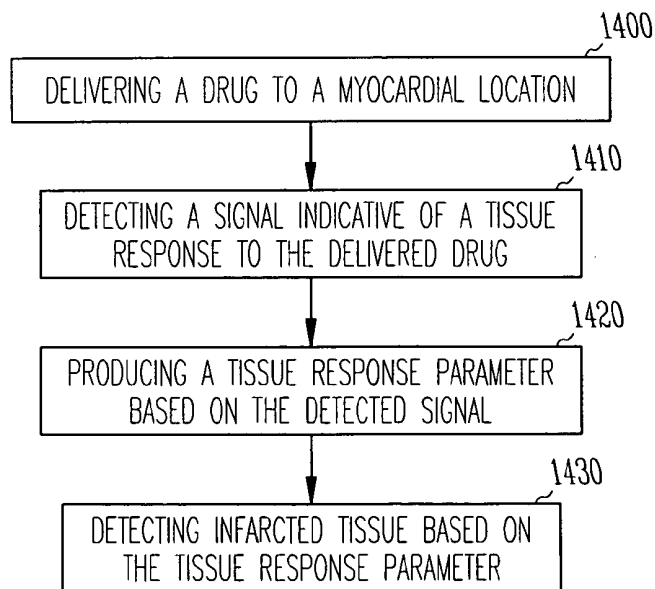


Fig.14

METHODS AND APPARATUSES FOR LOCALIZING MYOCARDIAL INFARCTION DURING CATHETERIZATION

FIELD OF THE INVENTION

This document generally relates to cardiac rhythm management systems and particularly, but not by way of limitation, to a system for localizing infarcted tissue in a heart having suffered myocardial infarction based on tissue properties that distinguish the infarcted tissue from normal myocardial tissue.

BACKGROUND

The heart is the center of a person's circulatory system. It includes an electro-mechanical system performing two major pumping functions. The heart includes four chambers: right atrium (RA), right ventricle (RV), left atrium (LA), and left ventricle (LV). The left portions of the heart, including LA and LV, draw oxygenated blood from the lungs and pump it to the organs of the body to provide the organs with their metabolic needs for oxygen. The right portions of the heart, including RA and RV, draw deoxygenated blood from the body organs and pump it to the lungs where the blood gets oxygenated. The efficiency of the pumping functions, indicative whether the heart is normal and healthy, is indicated by measures of hemodynamic performance, such as parameters related to intracardiac blood pressures and cardiac output.

In a normal heart, the sinoatrial node, the heart's natural pacemaker, generates electrical impulses, called action potentials, that propagate through an electrical conduction system to various regions of the heart to excite the myocardial tissues of these regions. Coordinated delays in the propagations of the action potentials in a normal electrical conduction system cause the various portions of the heart to contract in synchrony to result in efficient pumping functions indicated by a normal hemodynamic performance. A blocked or otherwise abnormal electrical conduction and/or deteriorated myocardial tissue cause dysynchronous contraction of the heart, resulting in poor hemodynamic performance, including a diminished blood supply to the heart and the rest of the body. The condition where the heart fails to pump enough blood to meet the body's metabolic needs is known as heart failure.

Myocardial infarction (MI) is the necrosis of portions of the myocardial tissue resulted from cardiac ischemia, a condition in which the myocardium is deprived of adequate oxygen and metabolite removal due to an interruption in blood supply. The necrotic tissue, known as infarcted tissue, loses the contractile properties of the normal, healthy myocardial tissue. Consequently, the overall contractility of the myocardium is weakened, resulting in decreased cardiac output. As a physiological compensatory mechanism that acts to increase cardiac output in response to MI, the LV diastolic filling pressure increases as the pulmonary and venous blood volume increases. This increases the LV preload (stress on the LV wall before its contracts to eject blood). One consequence is the progressive change of the LV shape and size, a process referred to as remodeling. Remodeling is initiated in response to a redistribution of cardiac stress and strain caused by the impairment of contractile function in the infarcted tissue as well as in nearby and/or interspersed viable myocardial tissue with lessened contractility due to the infarct. The remodeling starts with expansion of the region of the infarcted tissue and progresses to a chronic, global expansion in the size and change in the shape of the entire LV. Although the process is initiated by the compensatory mechanism that

increases cardiac output, the remodeling ultimately leads to further deterioration and dysfunction of the myocardium. Consequently, post MI patients experience impaired hemodynamic performance and have a significantly increased risk of developing heart failure.

For effectively and/or efficiently applying surgical or any other treatments to control the remodeling process, there is a need for localizing the infarcted tissue in a heart having suffered MI.

SUMMARY

A catheter with a tissue property sensor provides for localization of myocardial infarction (MI) by utilizing one or more differences between properties of infarcted myocardial tissue and properties of normal myocardial tissue. The tissue property sensor is to be placed on a cardiac wall during catheterization to sense at least one tissue property allowing for detection of MI.

In one embodiment, a system for localizing MI includes a catheter, a myocardial tissue property sensor, and a tissue property analyzer. The catheter includes a distal end configured for placement in a location on the cardiac wall. The myocardial tissue property sensor is incorporated into the distal end of the catheter to be placed in a myocardial location to sense a signal indicative of at least one tissue property. The tissue property analyzer includes an input to receive the sensed signal and an output indicative of whether the sensed signal indicates infarcted tissue.

Examples of the myocardial tissue property sensor include, but are not limited to, an optical sensor, an acoustic sensor, a contractility sensor, a temperature sensor, and a drug response sensor. The optical sensor includes an optical transmitter to emit a light and an optical receiver to receive an optical signal related to the emitted light. The acoustic sensor includes an acoustic transmitter to emit an acoustic energy and an acoustic receiver to receive an acoustic signal related to the emitted acoustic energy. The contractility sensor includes an accelerometer array with a plurality of accelerometers to sense acceleration signals related to displacement of the cardiac wall. The temperature sensor includes a thermal transmitter to emit a thermal energy and a thermometer to sense a temperature signal related to the emitted thermal energy. The drug response sensor includes a drug delivery device to deliver a drug and a drug response detector to detect a drug response signal. The optical signal, acoustic signal, acceleration signals, temperature signal, and drug response signal each indicates a tissue property allowing for detection of infarcted tissue.

In one embodiment, the tissue property analyzer includes a parameter generator and a comparator. The parameter generator produces a parameter based on the sensed signal. The comparator compares the parameter to a predetermined threshold and indicates a detection of infarcted tissue based on the comparison.

In one embodiment, the myocardial tissue property sensor is incorporated into the distal end of the catheter to be placed in a plurality of myocardial locations, one at a time, over a portion of the cardiac wall to sense signals each indicative of the tissue property for one of the myocardial locations. The tissue property analyzer includes a tissue property mapping module that produces a tissue property map presenting a measure of the tissue property over the portion of the cardiac wall based on the sensed signals.

In one embodiment, methods for localizing MI are provided. A sensor is placed in a myocardial location. A signal is sensed using to sensor to indicate at least one tissue property

in the myocardial location. Infarcted tissue is detected based on the signal. Examples of the signal include, but are not limited to, an optical signal, an acoustic signal, a signal indicative of myocardial contractility, a temperature signal, and a signal indicative of a myocardial tissue response to a drug delivery. These signals each indicates a tissue property allowing for detection of the infarcted tissue.

This Summary is an overview of some of the teachings of the present application and not intended to be an exclusive or exhaustive treatment of the present subject matter. Further details about the present subject matter are found in the detailed description and appended claims. Other aspects of the invention will be apparent to persons skilled in the art upon reading and understanding the following detailed description and viewing the drawings that form a part thereof, each of which are not to be taken in a limiting sense. The scope of the present invention is defined by the appended claims and their equivalents.

BRIEF DESCRIPTION OF THE DRAWINGS

The drawings illustrate generally, by way of example, but not by way of limitation, various embodiments discussed in the present document. The drawing are for illustrative purposes only and not to scale nor anatomically accurate.

FIG. 1 is an illustration of one embodiment of a system providing for localization of MI during cardiac catheterization, in which the system is used for an endocardial application, and portions of an environment in which the system is used.

FIG. 2 is an illustration of another embodiment of the system providing for localization of MI during cardiac catheterization, in which the system is used for an epicardial application, and portions of an environment in which the system is used.

FIG. 3 is block diagram illustrating one embodiment of a circuit of the system providing for localization of MI during cardiac catheterization.

FIG. 4 is a flow chart illustrating one embodiment of a method for localizing MI during cardiac catheterization.

FIG. 5 is block diagram illustrating one specific embodiment of the circuit of the system providing for localization of MI in which an optical sensor is used.

FIG. 6 is a flow chart illustrating one specific embodiment of the method for localizing MI in which an optical signal is sensed.

FIG. 7 is block diagram illustrating another specific embodiment of the circuit of the system providing for localization of MI in which an acoustic sensor is used.

FIG. 8 is a flow chart illustrating another specific embodiment of the method for localizing MI in which an acoustic signal is sensed.

FIG. 9 is block diagram illustrating another specific embodiment of the circuit of the system providing for localization of MI in which a contractility sensor is used.

FIG. 10 is a flow chart illustrating another specific embodiment of the method for localizing MI in which a signal indicative of a myocardial contractility is sensed.

FIG. 11 is block diagram illustrating another specific embodiment of the circuit of the system providing for localization of MI in which a temperature sensor is used.

FIG. 12 is a flow chart illustrating another specific embodiment of the method for localizing MI in which a signal indicative of temperature is sensed.

FIG. 13 is block diagram illustrating another specific embodiment of the circuit of the system providing for localization of MI in which a drug response sensor is used.

FIG. 14 is a flow chart illustrating another specific embodiment of the method for localizing MI in which a signal indicative of a myocardial tissue response to a drug delivery is sensed.

DETAILED DESCRIPTION

In the following detailed description, reference is made to the accompanying drawings which form a part hereof, and in which is shown by way of illustration specific embodiments in which the invention may be practiced. These embodiments are described in sufficient detail to enable those skilled in the art to practice the invention, and it is to be understood that the embodiments may be combined, or that other embodiments may be utilized and that structural, logical and electrical changes may be made without departing from the spirit and scope of the present invention. The following detailed description provides examples, and the scope of the present invention is defined by the appended claims and their equivalents.

It should be noted that references to “an”, “one”, or “various” embodiments in this disclosure are not necessarily to the same embodiment, and such references contemplate more than one embodiment.

This document discusses, among other things, a method and system for localizing MI (i.e., identifying regions of infarcted tissue) based on myocardial tissue properties. After MI, various properties of the infarcted tissue change during the scar formation process. By sensing one or more tissue properties across a portion of the cardiac wall, infarcted regions are localized as areas where the one or more tissue properties are determined to be associated with infarcted tissue. The method and system are also useable for monitoring any effect of therapies delivered to control the post-MI remodeling process by treating the infarcted tissue.

FIGS. 1 and 2 illustrate two embodiments of a system 100 providing for localization of MI and portions of an environment in which system 100 is used. System 100 includes a catheter 120 that provides for localization of at least one infarcted region 102 in a heart 101 that has suffered MI. Heart 101 includes an endocardial wall 103 and an epicardial wall 104. Catheter 120 has a proximal end 121 and a distal end 122. A myocardial tissue property sensor 110 is incorporated into catheter 120 at distal end 122. In the embodiment illustrated in FIG. 1, myocardial tissue property sensor 110 is configured for placement in various locations or regions on endocardial surface 103. In the embodiment illustrated in FIG. 2, myocardial tissue property sensor 110 is configured for placement in various locations or regions on epicardial surface 104. Myocardial tissue property sensor 110 senses one or more signals indicative of myocardial tissue properties. Proximal end 121 is outside the body and connected to an external tissue property analyzer 130. Tissue property analyzer 130 analyzes the one or more signals sensed by myocardial tissue property sensor 110 to detect infarcted tissue. Catheter 120 provides for electrical and/or other connections between myocardial tissue property sensor 110 and tissue property analyzer 130 to allow transmission of the one or more sensed signals.

Myocardial tissue property sensor 110 is configured for placement in a location or a region on endocardial wall 103 and/or epicardial wall 104. In one embodiment, at least a portion of myocardial tissue property sensor 110 is configured for penetration into the myocardial tissue in the location or region on the cardiac wall including endocardial wall 103 and/or epicardial wall 104. The penetration allows sensing of tissue properties that must be achieved with a sensor in the

tissue and stabilization of the sensor in the location or region of the cardiac wall. Myocardial tissue property sensor **110**, including all of its embodiments discussed below, includes at least a portion configured for tissue penetration when such a penetration is considered necessary and/or adequate. In all discussions related to sensor placement below, “in a location on a cardiac wall,” “in a region on a cardiac wall,” and like expressions include penetration of at least a portion of myocardial tissue property sensor **110** into tissue when such a penetration is considered necessary and/or adequate. Whether such a penetration is considered necessary and/or adequate depends on the need for reliable sensing of tissue property and/or the need for stabilizing the placement of myocardial tissue property sensor **110** during sensing, as understood by any person skilled in the art of cardiac catheterization and tissue property sensing.

In one embodiment, catheter **120** is a catheter dedicated to MI localization by myocardial tissue property sensing. In another embodiment, myocardial tissue property sensor **110** is incorporated into a catheter used for other diagnostic and/or therapeutic purposes. Examples of catheter **120** in this embodiment include, but are not limited to, a catheter for assessment of hemodynamic function, a catheter for mapping of cardiovascular structure, a substance (such as pharmaceutical and biological agents) delivery catheter, an ablation catheter, a pacing lead, and a defibrillation lead. In one embodiment, as illustrated in FIG. 1, catheter **120** is configured for transvenous or transarterial catheterization with distal end **122** reaching endocardial wall **103**. In another embodiment, as illustrated in FIG. 2, catheter **120** is configured for intercostal catheterization with distal end **122** reaching epicardial wall **104**. In one specific embodiment, the intercostal catheterization is performed using a minimally invasive surgical technique. For example, a small incision is made on chest between two ribs. Catheter **120** is inserted through the incision into intercostal space to reach heart **101** under guidance provided with some imaging technique. In one embodiment, catheter **120** is configured to be suitable for transvenous, transarterial, and intercostal catheterization.

For all descriptions below, the term “myocardial” includes “endocardial” and “epicardial,” and the term “cardiac wall” includes “endocardial wall” and “epicardial wall.” For example, any “myocardial tissue property sensor” is configured as an “endocardial tissue property sensor” for endocardial placement over a portion of the myocardium in one embodiment, as illustrated in FIG. 1, and an “epicardial tissue property sensor” for epicardial placement over a portion of the myocardium in another embodiment, as illustrated in FIG. 2. A “myocardial location” includes a location on endocardial wall **103** or epicardial wall **104** or locations in myocardial tissue accessible through endocardial wall **103** or epicardial wall **104**.

FIG. 3 illustrates one embodiment of a circuit of system **100**. The circuit includes a myocardial tissue property sensor **310** and a tissue property analyzer **330**. Myocardial tissue property sensor **310** represents one embodiment of myocardial tissue property sensor **110**. Tissue property analyzer **330** represents one embodiment of tissue property analyzer **130**. A sensor link **324**, which couples myocardial tissue property sensor **310** and tissue property analyzer **330** via electrical and/or other connections, is included in catheter **120** and extends from proximal end **121** to distal end **122**.

Myocardial tissue property sensor **310** includes a sensor that senses at least one signal indicative of a tissue property that changes as a result of MI. Examples of myocardial tissue property sensor **310** include, but are not limited to, an optical sensor, an acoustic sensor, a temperature sensor, a contractil-

ity sensor, and a drug response sensor. These examples are discussed below with reference to FIGS. 5, 7, 9, 11, and 13. Tissue property analyzer **330** includes an input coupled to myocardial tissue property sensor **220** through sensor link **324** and an output indicating detection of infarcted tissue. In one embodiment, tissue property analyzer **330** includes a parameter generator and an MI detector. The parameter generator produces at least one parameter representative of the tissue property indicated by the sensed signal. The MI detector includes a comparator with a signal input receiving the parameter, a threshold input receiving a predetermined threshold, and an output indicating a detection of the infarcted tissue based on a comparison between the signal and the threshold. In a specific embodiment, the threshold is determined based on a study evaluating a patient population. In another embodiment, tissue property analyzer **330** includes a tissue property mapping module to produce a tissue property map presenting a measure of at least one tissue property over at least a portion of the cardiac wall. In a further embodiment, tissue property analyzer **330** includes an MI detector to detect one or more infarcted regions based on the tissue property map.

FIG. 4 is a flow chart illustrating one embodiment of a method for localizing MI during cardiac catheterization. In one specific embodiment, the method is performed with system **100** including the circuit of FIG. 3.

A catheter is introduced into a body to provide for access to the heart at **400**. The catheter includes a sensor at its end portion. The sensor is placed in a location on the cardiac wall at **410**. A signal indicative of at least one tissue property of the tissue in that myocardial location is sensed at **420**. The tissue property indicated by the sensed signal is a tissue property that changes as a result of MI and provides for distinction between normal and infarcted tissues. Examples of the sensed signal include, but are not limited to an optical signal, an acoustic signal, a signal indicative of myocardial contractility, a temperature signal, and a signal indicative of a myocardial tissue response to a drug delivery. These examples are further discussed below with reference to FIGS. 6, 8, 10, 12, and 14. The infarcted tissue is detected based on the sensed signal at **430**. The detection indicates that the tissue in the myocardial location where the sensor is placed is infarcted tissue.

In one embodiment, the sensor is moved to and placed in a plurality of myocardial locations, one at a time, within at least a portion of the cardiac wall to sense the signal at each of these locations. The signal sensed at each location indicates whether the tissue in that location is infarcted tissue. In one embodiment, a parameter representative of the tissue property for each location is produced and compared to a predetermined threshold value. Infarcted tissue is detected for each location based on an outcome of the comparison. In another embodiment, a tissue property map is produced to present a measure of the at least one tissue property over the at least the portion of the cardiac wall. Boundaries of one or more infarcted regions are identified based on the tissue property map.

EXAMPLE 1

System with Optical Sensor

FIG. 5 illustrates one specific embodiment of the circuit of system **100**. The circuit provides for localization of MI using an optical sensor. This circuit includes a myocardial tissue property sensor **510**, which is a specific embodiment of myocardial tissue property sensor **310**, and a tissue property analyzer **530**, which is a specific embodiment of tissue property

analyzer **330**. A sensor link **524**, which is a specific embodiment of sensor link **324**, couples myocardial tissue property sensor **510** and tissue property analyzer **530**.

Myocardial tissue property sensor **510** is an optical sensor including an optical transmitter **512** and an optical receiver **514**. Optical transmitter **512** emits a light into tissue in a myocardial location where myocardial tissue property sensor **510** is placed. The light includes a visible light, an infrared light, an ultraviolet light, or a combination of such lights. Optical receiver **514** receives an optical signal related to the emitted light while the light is being emitted. The optical signal includes fluorescence generated from myocardial tissue in response to the emitted light. The fluorescence has an optical spectrum including wavelengths (colors) being a function of the tissue property. Thus, the fluorescence generated from infarcted tissue includes wavelengths that are different from the wavelengths of the fluorescence generated from normal tissue. In one embodiment, to increase the signal-to-noise ratio of the optical signal including the fluorescence, a fluorescent dye sensitive to transmembrane potentials is injected through catheter **120**. In one specific embodiment, myocardial tissue property sensor **510** includes an injection device allowing the injection of the fluorescent dye. Catheter **120** includes a lumen allowing passage of the fluorescent dye through the catheter. In a further embodiment, to further increase the signal-to-noise ratio, subthreshold electrical stimuli, such as subthreshold pacing pulses, are delivered to the heart. The subthreshold electrical stimuli are electrical stimuli each having a stimulation amplitude that is below the threshold for myocardial tissue excitation. Myocardial tissue property sensor **510** includes at least one electrode allowing delivery of the electrical stimuli. In one specific embodiment, catheter **120** includes an electrical conductor allowing delivery of the electrical stimuli through the catheter.

Tissue property analyzer **530** includes a wavelength analyzer **532** and an MI detector **534**. Wavelength analyzer **532** produces an optical spectrum of the optical signal received by optical receiver **514**. MI detector **534** detects infarcted tissue based on the optical spectrum. In one embodiment, MI detector **534** detects the infarcted tissue when the optical spectrum differs from a template spectrum associated with normal tissue by a predetermined margin. In an alternative embodiment, MI detector **534** detects the infarcted tissue when the optical spectrum matches a template spectrum associated with known infarcted tissue within a predetermined margin. For example, NADH (the reduced form of Nicotinamide Adenine Dinucleotide) is a product of metabolism associated with myocardial ischemia. A template spectrum is thus obtained from an optical signal including fluorescence generated from tissue with elevated level of NADH. In these embodiments, the template spectrum and the predetermined margin are each determined based on a study evaluating a patient population. In another embodiment, MI detector **534** detects the infarcted tissue based on a substantial change in the optical spectrum when the optical sensor moves from one myocardial location to another myocardial location. A quantitative standard for the substantiality of the change is determined based on a study evaluating a patient population.

FIG. **6** is a flow chart illustrating one specific embodiment of the method for localizing MI. As a specific embodiment of steps **420** and **430** of FIG. **3**, infarcted tissue is detected by sensing an optical signal.

A light is emitted to a myocardial location in a heart at **600**. In one embodiment, a fluorescent dye sensitive to transmembrane potentials is also released to the myocardial location. In a further embodiment, electrical stimuli, such as pacing

pulses, are delivered to the heart. An optical signal related to the emitted light is received at **610**, while the light is being emitted. An optical spectrum of the received optical signal is produced at **620**. Infarcted tissue is detected for the myocardial location based on the optical spectrum at **630**. In one embodiment, the infarcted tissue is detected when the optical spectrum differs from a template spectrum associated with normal tissue by a predetermined margin. In an alternative embodiment, the infarcted tissue is detected when the optical spectrum matches a template spectrum associated with known infarcted tissue within a predetermined margin. In one embodiment, steps **600** through **620** are repeated for a plurality of myocardial locations. The infarcted tissue is detected based on the optical spectra produced all the myocardial locations. An infarcted tissue region includes one or more myocardial locations where the optical spectra for the adjacent myocardial locations are substantially different from the optical spectra for the one or more myocardial locations.

EXAMPLE 2

System with Acoustic Sensor

FIG. **7** illustrates another specific embodiment of the circuit of system **100**. The circuit provides for localization of MI using an acoustic sensor. This circuit includes a myocardial tissue property sensor **710**, which is another specific embodiment of myocardial tissue property sensor **310**, and a tissue property analyzer **730**, which is another specific embodiment of tissue property analyzer **330**. A sensor link **724**, which is another specific embodiment of sensor link **324**, couples myocardial tissue property sensor **710** and tissue property analyzer **730**.

Myocardial tissue property sensor **710** is an acoustic sensor including an acoustic transmitter **712** and an acoustic receiver **714**. Acoustic transmitter **712** emits an acoustic energy into tissue in a myocardial location where myocardial tissue property sensor **710** is placed. In one embodiment, acoustic transmitter **712** includes a speaker to transmit an audible sound pulse. In another embodiment, acoustic transmitter **712** includes an ultrasound transmitter to transmit an ultrasound pulse. In one embodiment, acoustic transmitter **712** includes a piezoelectric crystal. Acoustic receiver **714** receives an acoustic signal related to the emitted acoustic energy. The acoustic signal includes echoes of the audible sound pulse or the ultrasound pulse. As a result of the scar formation process, infarcted tissue is stiffer than normal tissue. The echoes from infarcted tissue have a pitch distinguishable from the pitch associated of normal tissue.

Tissue property analyzer **730** includes a frequency analyzer **732** and an MI detector **734**. Frequency analyzer **732** produces an acoustic spectrum of the received acoustic signal. MI detector **734** detects infarcted tissue based on the acoustic spectrum. In one embodiment, MI detector **734** detects the infarcted tissue when the acoustic spectrum differs from a template spectrum associated with normal tissue by a predetermined margin. In an alternative embodiment, MI detector **734** detects the infarcted tissue when the acoustic spectrum matches a template spectrum associated with known infarcted tissue within a predetermined margin. In these embodiments, the template spectrum and the predetermined margin are each determined based on a study evaluating a patient population. In another embodiment, MI detector **734** detects the infarcted tissue based on a substantial change in the acoustic spectrum when the acoustic sensor moves from one myocardial location to another myocardial location.

A quantitative standard for the substantiality of the change is determined based on a study evaluating a patient population.

FIG. 8 is a flow chart illustrating another specific embodiment of the method for localizing MI. As another specific embodiment of steps 420 and 430 of FIG. 3, infarcted tissue is detected by sensing an acoustic signal.

An acoustic energy is emitted to a myocardial location at 800. In one embodiment, the acoustic energy is in a form of an audible sound. In another embodiment, the acoustic energy is in a form of an ultrasound. An acoustic signal related to the emitted acoustic energy is received at 810. The acoustic signal includes echoes of the audible sound or ultrasound. An acoustic spectrum of the received acoustic signal is produced at 820. Infarcted tissue is detected based on the acoustic spectrum at 830. In one embodiment, the infarcted tissue is detected when the acoustic spectrum differs from a template spectrum associated with normal tissue by a predetermined margin. In an alternative embodiment, the infarcted tissue is detected when the acoustic spectrum matches a template spectrum associated with known infarcted tissue within a predetermined margin. In another embodiment, steps 800 through 820 are repeated for a plurality of myocardial locations. The infarcted tissue is detected based on the acoustic spectra produced for the plurality of myocardial locations. An infarcted tissue region includes one or more myocardial locations where the acoustic spectra for the adjacent myocardial locations are substantially different from the acoustic spectra for the one or more myocardial locations.

EXAMPLE 3

System with Contractility Sensor

FIG. 9 illustrates another specific embodiment of the circuit of system 100. The circuit provides for localization of MI using a contractility sensor. This circuit includes a myocardial tissue property sensor 910, which is another specific embodiment of myocardial tissue property sensor 310, and a tissue property analyzer 930, which is another specific embodiment of tissue property analyzer 330. A sensor link 924, which is another specific embodiment of sensor link 324, couples myocardial tissue property sensor 910 and tissue property analyzer 930.

Myocardial tissue property sensor 910 is a contractility sensor that senses one or more signals indicative of myocardial contractility in a myocardial region. In one embodiment, the contractility sensor includes an accelerometer array including a plurality of accelerometers 912A, 912B, . . . , and 912N to sense acceleration signals from a plurality of locations constituting the myocardial region.

Tissue property analyzer 930 includes a motion pattern analyzer 932, a mapping module 934, and an MI detector 936. Motion pattern analyzer 932 produces a cardiac wall motion pattern for the myocardial region based on the sensed one or more signals indicative of myocardial contractility in the myocardial region. Mapping module 932 produces a contractility map presenting cardiac wall motion patterns for a plurality of myocardial regions within at least a portion of a cardiac wall. MI detector 936 detects infarcted tissue based on the contractility map. Infarcted tissue regions are detected by identifying dyskinetic and/or hypokinetic regions on the contractility map.

FIG. 10 is a flow chart illustrating another specific embodiment of the method for localizing MI. As another specific embodiment of steps 420 and 430 of FIG. 3, infarcted tissue is detected by sensing a signal indicative of a myocardial contractility.

One or more signals indicative of myocardial contractility in a myocardial region is sensed at 1000. In one embodiment, this includes sensing a plurality of acceleration signals from the myocardial region. A cardiac wall motion pattern for the myocardial region is produced based on the sensed one or more signals at 1010. Steps 1000 and 1010 are repeated for a plurality of myocardial regions, and a contractility map presenting cardiac wall motion patterns for the plurality of myocardial regions is produced at 1020. Infarcted tissue is detected based on the contractility map at 1030. In one embodiment, the infarcted tissue is detected by identifying dyskinetic and/or hypokinetic regions on the contractility map. In one embodiment, infarcted tissue is detected by identifying myocardial regions associated with cardiac wall displacements that are substantially smaller than the cardiac wall displacements of other myocardial regions.

EXAMPLE 4

System with Temperature Sensor

FIG. 11 illustrates one specific embodiment of the circuit of system 100. The circuit provides for localization of MI using a temperature sensor. This circuit includes a myocardial tissue property sensor 1110, which is another specific embodiment of myocardial tissue property sensor 310, and a tissue property analyzer 1130, which is another specific embodiment of tissue property analyzer 330. A sensor link 1124, which is another specific embodiment of sensor link 324, couples myocardial tissue property sensor 1110 and tissue property analyzer 1130.

Myocardial tissue property sensor 1110 is a temperature sensor including a thermal transmitter 1112 and a thermometer 1114. Thermal transmitter 1112 emits a thermal energy into tissue in a myocardial location where myocardial tissue property sensor 1110 is placed. In one embodiment, the thermal energy raises the temperature at the myocardial location. In another embodiment, the thermal energy lowers the temperature at the cardiac wall location. In one embodiment, myocardial tissue property sensor 1110 includes an injection device allowing injection of a thermal dilution liquid. In one specific embodiment, catheter 120 includes a lumen allowing passage of thermal dilution liquid. Thermometer 1114 senses a temperature related to the emitted thermal energy.

Tissue property analyzer 1130 includes a thermal perfusion analyzer 1132 and an MI detector 1134. Thermal perfusion analyzer 1132 produces a rate of temperature change (or thermal perfusion rate) being a change in the sensed temperature over a predetermined period of time. Infarcted tissue includes tissue properties related to thermal perfusion that are distinguishable from those of normal tissue. MI detector 1134 detects infarcted tissue based on the rate of temperature change. In one embodiment, MI detector 1134 detects the infarcted tissue when the rate of temperature change differs from a template rate associated with normal tissue by a predetermined margin. In an alternative embodiment, MI detector 1134 detects the infarcted tissue when the rate of temperature change matches a template spectrum associated with known infarcted tissue within a predetermined margin. In these embodiments, the template rate and the predetermined margin are each determined based on a study evaluating a patient population. In another embodiment, MI detector 1134 detects the infarcted tissue based on a substantial change in the rate of temperature change when the acoustic sensor moves from one myocardial location to another myocardial

location. A quantitative standard for the substantiality of the change is determined based on a study evaluating a patient population.

FIG. 12 is a flow chart illustrating another specific embodiment of the method for localizing MI. As another specific embodiment of steps 420 and 430 of FIG. 3, infarcted tissue is detected by sensing a signal indicative of temperature.

A thermal energy is emitted to a myocardial location at 1200. In one embodiment, the thermal energy is emitted to heat the tissue in the myocardial location. In another embodiment, the thermal energy is emitted to cool the tissue in the myocardial location. In one embodiment, a thermal dilution liquid is released to the myocardial location. A temperature related to the emitted thermal energy is sensed at 1210, following the emission of the thermal energy. A rate of temperature change, or thermal perfusion rate, which is a change in the sensed temperature over a predetermined period of time, is measured for the myocardial location at 1220. Infarcted tissue is detected based on the rate of temperature change at 1230. In one embodiment, the infarcted tissue is detected when the rate of temperature change differs from a template rate associated with normal tissue by a predetermined margin. In an alternative embodiment, the infarcted tissue is detected when the rate of temperature change matches a template rate associated with known infarcted tissue within a predetermined margin. In another embodiment, steps 1200 through 1220 are repeated for a plurality of myocardial locations. The infarcted tissue is detected based on the rates of temperature change measured for the plurality of myocardial locations. An infarcted tissue region includes one or more myocardial locations where the rates of temperature change for the adjacent myocardial locations are substantially different from the rates of temperature change for the one or more myocardial locations.

EXAMPLE 5

System with Drug Response Sensor

FIG. 13 illustrates another specific embodiment of the circuit of system 100. The circuit provides for localization of MI using a drug response sensor. This circuit includes a myocardial tissue property sensor 1310, which is another specific embodiment of myocardial tissue property sensor 310, and a tissue property analyzer 1330, which is another specific embodiment of tissue property analyzer 330. A sensor link 1324, which is another specific embodiment of sensor link 324, couples myocardial tissue property sensor 1310 and tissue property analyzer 1330.

Myocardial tissue property sensor 1310 is a drug response sensor including a drug delivery device 1312 and a drug response detector 1314. Drug delivery device 1312 releases a drug from a myocardial location where myocardial tissue property sensor 1310 is placed. The drug is of a type that causes a reaction from infarcted tissue that is distinguishable from a reaction from normal tissue. Examples of the drug include, but are not limited to, isoproterenol, dobutamine, nitroglycerin, and brain natriuretic peptide (BNP). In one embodiment, catheter 120 includes a lumen allowing passage of the drug from proximal end 121 to drug delivery device 1312. Drug response detector 1314 detects a signal indicative of a tissue response the delivered drug.

Tissue property analyzer 1330 includes a drug response analyzer 1332 and an MI detector 1334. Drug response analyzer 1332 produces a tissue response parameter as a tissue response parameter to the delivered drug based on the signal detected by drug response detector 1314. MI detector 1334

detects infarcted tissue based on the tissue response parameter to the delivered drug. In one embodiment, MI detector 1334 detects the infarcted tissue when the tissue response parameter differs from a template tissue response parameter associated with normal tissue by a predetermined margin. In an alternative embodiment, MI detector 1334 detects the infarcted tissue when the tissue response parameter matches a template tissue response parameter associated with known infarcted tissue within a predetermined margin. In these embodiments, the template tissue response parameter and the predetermined margin are each determined based on a study evaluating a patient population. In another embodiment, MI detector 1334 detects the infarcted tissue based on a substantial change in the tissue response parameter when the acoustic sensor moves from one myocardial location to another myocardial location. A quantitative standard for the substantiality of the change is determined based on a study evaluating a patient population.

In one specific embodiment, the drug includes an agent changing the contractility of myocardial tissue, such as isoproterenol. Drug response detector 1314 includes a contractility sensor to sense a signal indicative of myocardial contractility, such as an accelerometer. Drug response analyzer 1332 produces a parameter indicative of the myocardial contractility. In one embodiment, drug response analyzer 1332 includes a displacement analyzer to produce a parameter indicative of a cardiac wall displacement based on the acceleration signal sensed by the accelerometer. MI detector 1334 detects infarcted tissue based on the myocardial contractility, such as indicated by the parameter indicative of the cardiac wall displacement.

In another specific embodiment, the drug includes an agent known to produce a rapid, even perfusion in tissue, such as nitroglycerin. Drug response detector 1314 includes a drug concentration sensor. Drug response analyzer 1332 includes a drug perfusion analyzer that produces a rate of drug perfusion, which is a change in the sensed drug concentration over a predetermined period of time. MI detector 1334 detects the infarcted tissue based on the rate of drug perfusion.

FIG. 14 is a flow chart illustrating another specific embodiment of the method for localizing MI. As another specific embodiment of steps 420 and 430 of FIG. 3, infarcted tissue is detected by sensing a signal indicative of a myocardial tissue response to a drug delivery.

A drug is delivered to a myocardial location at 1400. The drug provides for detection of infarcted tissue by examining a tissue property that is sensitive to the drug. Examples of the drug include, but are not limited to, isoproterenol, dobutamine, nitroglycerin, and BNP. A signal indicative of a tissue response to the delivered drug is detected at 1410. A tissue response parameter is produced based on the signal indicative of the tissue response at 1420. Infarcted tissue is detected for the myocardial region based on the tissue response parameter at 1430. In one embodiment, the infarcted tissue is detected when the tissue response parameter differs from a template tissue response parameter associated with normal tissue by a predetermined margin. In an alternative embodiment, the infarcted tissue is detected when the tissue response parameter matches a template tissue response parameter associated with known infarcted tissue within a predetermined margin. In another embodiment, steps 1400 and 1510 are repeated for a plurality of myocardial locations. The infarcted tissue is detected based on the tissue response parameters detected for the plurality of myocardial locations. An infarcted tissue region includes one or more myocardial locations where the tissue response parameters detected from

the adjacent myocardial locations are substantially different from the tissue response parameters detected from the one or more myocardial locations.

In one specific embodiment, the drug includes an agent changing the contractility of myocardial tissue, such as nitroglycerin. The tissue response is indicated by a signal indicative of myocardial contractility, such as an acceleration sensed from the cardiac wall. Infarcted tissue is generally less sensitive to the agent than normal tissue. That is, the agent causes a smaller change in contractility in infarcted tissue than in normal tissue. The infarcted tissue is detected based on the signal indicative of myocardial contractility.

In another specific embodiment, the drug includes an agent known to perfuse rapidly and evenly in tissue, such as nitroglycerin. A drug concentration is sensed following the delivery of the drug. A rate of drug perfusion, which is a change in the sensed drug concentration over a predetermined period of time, is measured. Infarcted tissue is generally more resistant to the perfusion of the agent than normal tissue. The infarcted tissue is detected based on the rate of drug perfusion.

In General

It is to be understood that the above detailed description, including Examples 1 through 5, is intended to be illustrative, and not restrictive. For example, myocardial tissue property sensor **110** includes any sensor or sensors capable of sensing a signal indicative of a myocardial tissue property that changes as a result of MI. Tissue property analyzer **130** detects infarcted tissue generally by analyzing that signal. Other embodiments, including any possible permutation of the system components discussed in this document, will be apparent to those of skill in the art upon reading and understanding the above description. The scope of the invention should, therefore, be determined with reference to the appended claims, along with the full scope of equivalents to which such claims are entitled.

What is claimed is:

1. A system for localizing myocardial infarction (MI) in a heart having a cardiac wall, the system comprising:

a transvenous catheter including a proximal end, a distal end, and a sensor link extending from the proximal end and the distal end, the distal end configured for endocardial placement on the cardiac wall;

a myocardial tissue property sensor incorporated into the distal end of the catheter, the myocardial tissue property sensor adapted to be placed in a plurality of locations, one at a time, over at least a portion of the cardiac wall to sense signals each indicative of at least one tissue property associated with one of the plurality of locations and each changing as a result of MI, the myocardial tissue property sensor including an optical sensor adapted to emit a light and receive the sensed signals; and

a tissue property analyzer configured to be connected to the proximal end of the catheter and coupled to the myocardial tissue property sensor via electrical connections of the sensor link, the tissue property analyzer adapted to produce a tissue property map presenting a measure of the at least one tissue property over the at least the portion of the cardiac wall using the sensed signals and further adapted to detect one or more infarcted regions using the tissue property map and a template spectrum associated with known infarcted tissue.

2. The system of claim **1**, wherein the catheter comprises a diagnostic catheter adapted for assessment of hemodynamic function.

3. The system of claim **1**, wherein the catheter comprises a diagnostic catheter adapted for mapping of cardiovascular structure.

4. The system of claim **1**, wherein the catheter comprises a substance-delivery catheter.

5. The system of claim **1**, wherein the catheter comprises an ablation catheter.

6. The system of claim **1**, wherein the catheter comprises a pacing lead.

7. The system of claim **1**, wherein the catheter comprises a defibrillation lead.

8. A system for localizing myocardial infarction (MI) in a heart having a cardiac wall, the system comprising:

a catheter including a proximal end, a distal end, and a sensor link extending from the proximal end and the distal end, the distal end configured for placement on the cardiac wall;

a myocardial tissue property sensor incorporated into the distal end of the catheter and adapted to be placed on the cardiac wall, the myocardial tissue property sensor including an optical sensor including:

an optical transmitter to emit a light; and

an optical receiver to receive an optical signal related to the emitted light, the optical signal indicative of a tissue property that changes as a result of MI; and

a tissue property analyzer adapted to be coupled to the proximal end of the catheter and including:

a wavelength analyzer adapted to produce an optical spectrum of the optical signal; and

an MI detector adapted to detect infarcted tissue by comparing the optical spectrum to a template spectrum obtained from an optical signal including fluorescence generated from tissue with elevated level of NADH; and

wherein the sensor link is configured to couple the myocardial tissue property sensor to the tissue property analyzer using electrical connections.

9. The system of claim **8**, wherein the catheter comprises a lumen allowing injection of a fluorescent dye through the lumen, the fluorescent dye sensitive to transmembrane potentials.

10. The system of claim **9**, wherein the catheter comprises a lead extending through at least a portion of the catheter and an electrode at or near the distal end, the electrode connected to the lead to allow delivery of electrical stimuli.

11. A system for localizing myocardial infarction (MI), the system comprising:

a transvenous catheter including a proximal end, a distal end, and a sensor link extending from the proximal end and the distal end, the distal end configured for endocardial placement;

a myocardial tissue property sensor incorporated into the distal end of the catheter, the myocardial tissue property sensor adapted to be placed in an endocardial location on a portion of an endocardial wall and including an optical sensor adapted to emit a light to the endocardial location and receive an optical signal related to the emitted light and indicative of at least one tissue property that changes as a result of MI in the endocardial; and

a tissue property analyzer adapted to be coupled to the proximal end of the catheter to receive the optical signal received by the optical sensor, the tissue property analyzer adapted to produce an optical spectrum of the received optical signal and further adapted to detect infarcted tissue by comparing the optical spectrum of the received optical signal to a template spectrum obtained

from an optical signal including fluorescence generated from tissue with elevated level of NADH, wherein the sensor link is configured to couple the myocardial tissue property sensor to the tissue property analyzer via electrical connections.

12. The system of claim 11, wherein the catheter comprises a lumen allowing injection of a fluorescent dye through the lumen, the fluorescent dye sensitive to transmembrane potentials.

13. The system of claim 12, wherein the catheter comprises a lead extending through at least a portion of the catheter and an electrode at or near the distal end, the electrode connected to the lead to allow delivery of electrical stimuli.

14. A system for localizing myocardial infarction (MI), the system comprising:

a transvenous catheter including a proximal end, a distal end, and a sensor link extending from the proximal end and the distal end, the distal end configured for endocardial placement;

a myocardial tissue property sensor adapted to sense an optical signal indicative of at least one tissue property that changes as a result of MI, the myocardial tissue property sensor incorporated into the distal end of the catheter and adapted to be placed in a plurality of endocardial locations, one at a time, over at least a portion of an endocardial wall to sense optical signals each indicative of the at least one tissue property for one of the plurality of endocardial locations; and

a tissue property analyzer adapted to be connected to the proximal end of the catheter and receive the sensed optical signals via electrical connections of the sensor link, the tissue property analyzer including:

a tissue property mapping module adapted to produce a tissue property map presenting a measure of the at least one tissue property over at least the portion of the endocardial wall based on the sensed optical signals; and

an MI detector adapted to detect one or more infarcted regions based on the tissue property map and a template spectrum obtained from an optical signal including fluorescence generated from tissue with elevated level of NADH.

15. The system of claim 14, wherein the catheter comprises a lead extending through at least a portion of the catheter and an electrode at or near the distal end, the electrode connected to the lead to allow delivery of electrical stimuli.

16. The system of claim 15, wherein the optical sensor comprises:

an optical transmitter to emit a light; and
an optical receiver to receive an optical signal related to the emitted light.

17. A method for localizing myocardial infarction (MI) in a heart having an endocardial wall, the method comprising:

introducing a transvenous catheter including a proximal end, a distal end, and an optical sensor incorporated into the distal end by transvenous catheterization to provide for access to the endocardial wall of the heart;

placing the optical sensor in endocardial locations over a portion of the endocardial wall;

sensing optical signals in the endocardial locations using the optical sensor, the optical signals each indicative of at least one tissue property associated with the endocardial locations;

receiving the sensed optical signals using a tissue property analyzer via electrical connections coupling the optical sensor to the tissue property analyzer, the tissue property analyzer connected to the proximal end of the catheter; producing parameters based on the received sensed signals using the tissue property analyzer, the parameters representative of the at least one tissue property for the endocardial locations producing a tissue property map using the tissue property analyzer, the tissue property map presenting the parameters representative of the at least one tissue property over the portion of the endocardial wall; and

detecting one or more infarcted regions based on the tissue property map using the the parameters and a template spectrum obtained from an optical signal including fluorescence generated from tissue with elevated level of NADH.

18. The method of claim 17, wherein detecting the one or more infarcted regions comprises identifying where substantial changes in the parameter representative of the at least one tissue property occur on the tissue property map.

19. A method for localizing myocardial infarction (MI) in a heart, the method comprising:

introducing a transvenous catheter including an optical sensor by transvenous catheterization to provide for access to the heart;

placing the optical sensor in an endocardial location in the heart;

emitting a light from the optical sensor;

receiving an optical signal related to the emitted light, the optical signal indicative of a tissue property in the endocardial location;

producing an optical spectrum of the received optical signal;

obtaining a template spectrum associated with known infarcted tissue from an optical signal including fluorescence generated from tissue with elevated level of NADH; and

detecting infarcted tissue by comparing the optical spectrum to the template spectrum.

20. The method of claim 19, further comprising injecting a fluorescent dye sensitive to transmembrane potentials to the endocardial location.

21. The method of claim 19, further comprising delivering subthreshold electrical stimuli to the endocardial location.

22. The method of claim 19, wherein detecting the infarcted tissue comprises detecting the infarcted tissue when the optical spectrum matches the template spectrum within a predetermined margin.

23. The method of claim 19, further comprising repeating the emitting the light, receiving the optical signal, and producing the optical spectrum for a plurality of endocardial locations, wherein detecting the infarcted tissue comprises detecting the infarcted tissue based on the optical spectra produced for the plurality of endocardial locations.

* * * * *

UNITED STATES PATENT AND TRADEMARK OFFICE
CERTIFICATE OF CORRECTION

PATENT NO. : 7,640,046 B2
APPLICATION NO. : 10/871865
DATED : December 29, 2009
INVENTOR(S) : Pastore et al.

Page 1 of 1

It is certified that error appears in the above-identified patent and that said Letters Patent is hereby corrected as shown below:

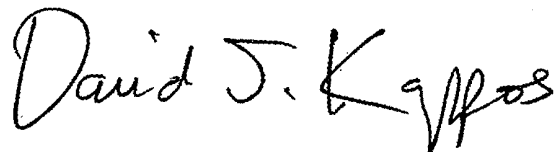
On the Title Page:

The first or sole Notice should read --

Subject to any disclaimer, the term of this patent is extended or adjusted under 35 U.S.C. 154(b) by 370 days.

Signed and Sealed this

Twenty-first Day of December, 2010

A handwritten signature in black ink that reads "David J. Kappos". The signature is written in a cursive, flowing style.

David J. Kappos
Director of the United States Patent and Trademark Office

专利名称(译)	用于在导管插入术中定位心肌梗塞的方法和装置		
公开(公告)号	US7640046	公开(公告)日	2009-12-29
申请号	US10/871865	申请日	2004-06-18
[标]申请(专利权)人(译)	PASTORE JOSEPH中号 吉鲁阿尔史蒂芬δ		
申请(专利权)人(译)	PASTORE JOSEPH中号 吉鲁阿尔史蒂芬δ		
当前申请(专利权)人(译)	心脏起搏器, INC.		
[标]发明人	PASTORE JOSEPH M GIROUARD STEVEN D		
发明人	PASTORE, JOSEPH M. GIROUARD, STEVEN D.		
IPC分类号	A61B5/00 G01N21/00 G01N21/62 A61B5/0265 A61B5/11 A61B8/12 A61N1/362 A61N1/37		
CPC分类号	A61B5/0084 A61B5/0265 A61B5/1107 A61B8/12 A61N1/3702 A61B5/4839 A61B5/0071 A61B5/6869 A61B2562/0219		
其他公开文献	US20050283195A1		
外部链接	Espacenet USPTO		

摘要(译)

具有组织特性传感器的导管通过利用梗塞心肌组织的特性和正常心肌组织的特性之间的一个或多个差异来提供心肌梗塞 (MI) 的定位。在导管插入期间将组织特性传感器放置在心内膜壁或心外膜壁上以感测至少一种允许检测MI的组织特性。组织特性传感器的示例包括但不限于光学传感器, 声学传感器, 收缩性传感器, 温度传感器和药物响应传感器。在一个实施例中, 组织特性传感器感测心内膜壁或心外膜壁上的各个位置的组织特性, 并检测指示梗塞组织和正常组织之间的边界的组织特性的实质变化。

