



US007295866B2

(12) **United States Patent**  
**Al-Ali**

(10) **Patent No.:** **US 7,295,866 B2**  
(45) **Date of Patent:** **Nov. 13, 2007**

(54) **LOW POWER PULSE OXIMETER**

(75) Inventor: **Ammar Al-Ali**, Tustin, CA (US)

(73) Assignee: **Masimo Corporation**, Irvine, CA (US)

(\*) Notice: Subject to any disclaimer, the term of this patent is extended or adjusted under 35 U.S.C. 154(b) by 527 days.

(21) Appl. No.: **10/785,573**

(22) Filed: **Feb. 24, 2004**

(65) **Prior Publication Data**

US 2004/0181133 A1 Sep. 16, 2004

**Related U.S. Application Data**

(63) Continuation of application No. 10/184,028, filed on Jun. 26, 2002, now Pat. No. 6,697,658.

(60) Provisional application No. 60/302,564, filed on Jul. 2, 2001.

(51) **Int. Cl.**  
**A61B 5/00** (2006.01)

(52) **U.S. Cl.** ..... **600/323; 600/310**

(58) **Field of Classification Search** ..... **600/310, 600/322, 323, 333, 336**

See application file for complete search history.

(56) **References Cited**

**U.S. PATENT DOCUMENTS**

4,960,128 A	10/1990	Gordon et al.
4,964,408 A	10/1990	Hink et al.
5,041,187 A	8/1991	Hink et al.
5,069,213 A	12/1991	Polczynski
5,163,438 A	11/1992	Gordon et al.
5,337,744 A	8/1994	Branigan
D353,195 S	12/1994	Savage et al.
D353,196 S	12/1994	Savage et al.
5,431,170 A	7/1995	Mathews
D361,840 S	8/1995	Savage et al.
D362,063 S	9/1995	Savage et al.

5,452,717 A	9/1995	Branigan et al.
D363,120 S	10/1995	Savage et al.
5,482,036 A	1/1996	Diab et al.
5,490,505 A	2/1996	Diab et al.
5,494,043 A	2/1996	O'Sullivan et al.
5,533,511 A	7/1996	Kaspari et al.
5,562,002 A	10/1996	Lalin
5,590,649 A	1/1997	Caro et al.
5,602,924 A	2/1997	Durand et al.
5,632,272 A	5/1997	Diab et al.
5,638,816 A	6/1997	Kiani-Azarbayjany et al.
5,638,818 A	6/1997	Diab et al.

(Continued)

**FOREIGN PATENT DOCUMENTS**

EP 0 872 210 A1 10/1998

(Continued)

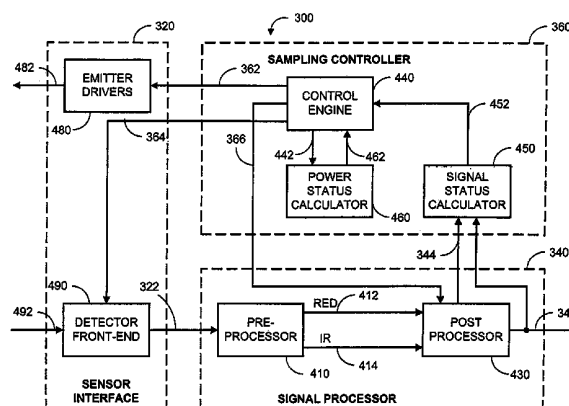
*Primary Examiner*—Eric F. Winakur

(74) *Attorney, Agent, or Firm*—Knobbe, Martens, Olson & Bear LLP

(57) **ABSTRACT**

A pulse oximeter adaptively samples an input signal from a sensor in order to reduce power consumption in the absence of overriding conditions. Various sampling mechanisms may be used individually or in combination, including reducing the duty cycle of a drive current to a sensor emitter, intermittently powering-down a front-end interface to a sensor detector, or increasing the time shift between processed data blocks. Both internal parameters and output parameters may be monitored to trigger or override a reduced power consumption state. In this manner, a pulse oximeter can lower power consumption without sacrificing performance during, for example, high noise conditions or oxygen desaturations.

**33 Claims, 11 Drawing Sheets**



## U.S. PATENT DOCUMENTS

5,645,440	A	7/1997	Tobler et al.	6,632,181	B2	10/2003	Flaherty et al.
5,685,299	A	11/1997	Diab et al.	6,640,116	B2	10/2003	Diab
D393,830	S	4/1998	Tobler et al.	6,643,530	B2	11/2003	Diab et al.
5,743,262	A	4/1998	Lepper, Jr. et al.	6,650,917	B2	11/2003	Diab et al.
5,758,644	A	6/1998	Diab et al.	6,654,624	B2	11/2003	Diab et al.
5,760,910	A	6/1998	Lepper, Jr. et al.	6,658,276	B2	12/2003	Kiani et al.
5,769,785	A	6/1998	Diab et al.	6,661,161	B1	12/2003	Lanzo et al.
5,782,757	A	7/1998	Diab et al.	6,671,531	B2	12/2003	Al-Ali et al.
5,785,659	A	7/1998	Caro et al.	6,678,543	B2	1/2004	Diab et al.
5,791,347	A	8/1998	Flaherty et al.	6,684,090	B2	1/2004	Ali et al.
5,810,734	A	9/1998	Caro et al.	6,684,091	B2	1/2004	Parker
5,823,950	A	10/1998	Diab et al.	6,697,656	B1	2/2004	Al-Ali
5,830,131	A	11/1998	Caro et al.	6,697,658	B2 *	2/2004	Al-Ali ..... 600/323
5,833,618	A	11/1998	Caro et al.	RE38,476	E	3/2004	Diab et al.
5,860,919	A	1/1999	Kiani-Azarbayjany et al.	6,699,194	B1	3/2004	Diab et al.
5,890,929	A	4/1999	Mills et al.	6,714,804	B2	3/2004	Al-Ali et al.
5,904,654	A	5/1999	Wohltmann et al.	RE38,492	E	4/2004	Diab et al.
5,919,134	A	7/1999	Diab	6,721,585	B1	4/2004	Parker
5,924,979	A	7/1999	Swedlow et al.	6,725,075	B2	4/2004	Al-Ali
5,934,925	A	8/1999	Tobler et al.	6,735,459	B2	5/2004	Parker
5,940,182	A	8/1999	Lepper, Jr. et al.	6,745,060	B2	6/2004	Diab et al.
5,995,855	A	11/1999	Kiani et al.	6,760,607	B2	7/2004	Al-Ali
5,997,343	A	12/1999	Mills et al.	6,770,028	B1	8/2004	Ali et al.
6,002,952	A	12/1999	Diab et al.	6,771,994	B2	8/2004	Kiani et al.
6,011,986	A	1/2000	Diab et al.	6,792,300	B1	9/2004	Diab et al.
6,027,452	A	2/2000	Flaherty et al.	6,813,511	B2	11/2004	Diab et al.
6,036,642	A	3/2000	Diab et al.	6,816,741	B2	11/2004	Diab
6,045,509	A	4/2000	Caro et al.	6,822,564	B2	11/2004	Al-Ali
6,067,462	A	5/2000	Diab et al.	6,826,419	B2	11/2004	Diab et al.
6,081,735	A	6/2000	Diab et al.	6,830,711	B2	12/2004	Mills et al.
6,088,607	A	7/2000	Diab et al.	6,850,787	B2	2/2005	Weber et al.
6,110,522	A	8/2000	Lepper, Jr. et al.	6,850,788	B2	2/2005	Al-Ali
6,144,868	A	11/2000	Parker	6,852,083	B2	2/2005	Caro et al.
6,151,516	A	11/2000	Kiani-Azarbayjany et al.	6,861,639	B2	3/2005	Al-Ali
6,152,754	A	11/2000	Gerhardt et al.	6,898,452	B2	5/2005	Al-Ali et al.
6,157,850	A	12/2000	Diab et al.	6,920,345	B2	7/2005	Al-Ali et al.
6,165,005	A	12/2000	Mills et al.	6,931,268	B1	8/2005	Kiani-Azarbayjany et al.
6,184,521	B1	2/2001	Coffin, IV et al.	6,934,570	B2	8/2005	Kiani et al.
6,206,830	B1	3/2001	Diab et al.	6,939,305	B2	9/2005	Flaherty et al.
6,229,856	B1	5/2001	Diab et al.	6,943,348	B1	9/2005	Coffin IV
6,236,872	B1	5/2001	Diab et al.	6,950,687	B2	9/2005	Al-Ali
6,256,523	B1	7/2001	Diab et al.	6,961,598	B2	11/2005	Diab
6,263,222	B1	7/2001	Diab et al.	6,970,792	B1	11/2005	Diab
6,278,522	B1	8/2001	Lepper, Jr. et al.	6,979,812	B2	12/2005	Al-Ali
6,280,213	B1	8/2001	Tobler et al.	6,985,764	B2	1/2006	Mason et al.
6,285,896	B1	9/2001	Tobler et al.	6,993,371	B2	1/2006	Kiani et al.
6,321,100	B1	11/2001	Parker	6,996,427	B2	2/2006	Ali et al.
6,334,065	B1	12/2001	Al-Ali et al.	6,999,904	B2	2/2006	Weber et al.
6,343,224	B1	1/2002	Parker	7,003,338	B2	2/2006	Weber et al.
6,349,228	B1	2/2002	Kiani et al.	7,003,339	B2	2/2006	Diab et al.
6,360,114	B1	3/2002	Diab et al.	7,015,451	B2	3/2006	Dalke et al.
6,371,921	B1	4/2002	Caro et al.	7,024,233	B2	4/2006	Al et al.
6,377,829	B1	4/2002	Al-Ali	7,027,849	B2	4/2006	Al-Ali
6,388,240	B2	5/2002	Schulz et al.	7,030,749	B2	4/2006	Al-Ali
6,397,091	B2	5/2002	Diab et al.	7,039,449	B2	5/2006	Al-Ali
6,430,525	B1	8/2002	Weber et al.	7,041,060	B2	5/2006	Flaherty et al.
6,463,311	B1	10/2002	Diab	7,044,918	B2	5/2006	Diab
6,470,199	B1	10/2002	Kopotic et al.	7,067,893	B2	6/2006	Mills et al.
6,501,975	B2	12/2002	Diab et al.	7,096,052	B2	8/2006	Mason et al.
6,515,273	B2	2/2003	Al-Ali	7,096,054	B2	8/2006	Abdul-Hafiz et al.
6,519,487	B1	2/2003	Parker	7,132,641	B2	11/2006	Schulz et al.
6,525,386	B1	2/2003	Mills et al.	7,142,901	B2	11/2006	Kiani et al.
6,526,300	B1	2/2003	Kiani et al.	7,149,561	B2	12/2006	Diab
6,541,756	B2	4/2003	Schulz et al.	7,186,966	B2	3/2007	Al-Ali
6,542,764	B1	4/2003	Al-Ali et al.	7,190,261	B2	3/2007	Al-Ali
6,580,086	B1	6/2003	Schulz et al.	2003/0218386	A1	11/2003	Dalke et al.
6,584,336	B1	6/2003	Ali et al.	2005/0234317	A1	10/2005	Kiani
6,595,316	B2	7/2003	Cybulski et al.				
6,597,933	B2	7/2003	Kiani et al.				
6,606,511	B1	8/2003	Ali et al.				

## FOREIGN PATENT DOCUMENTS

WO WO99/63883 12/1999

\* cited by examiner

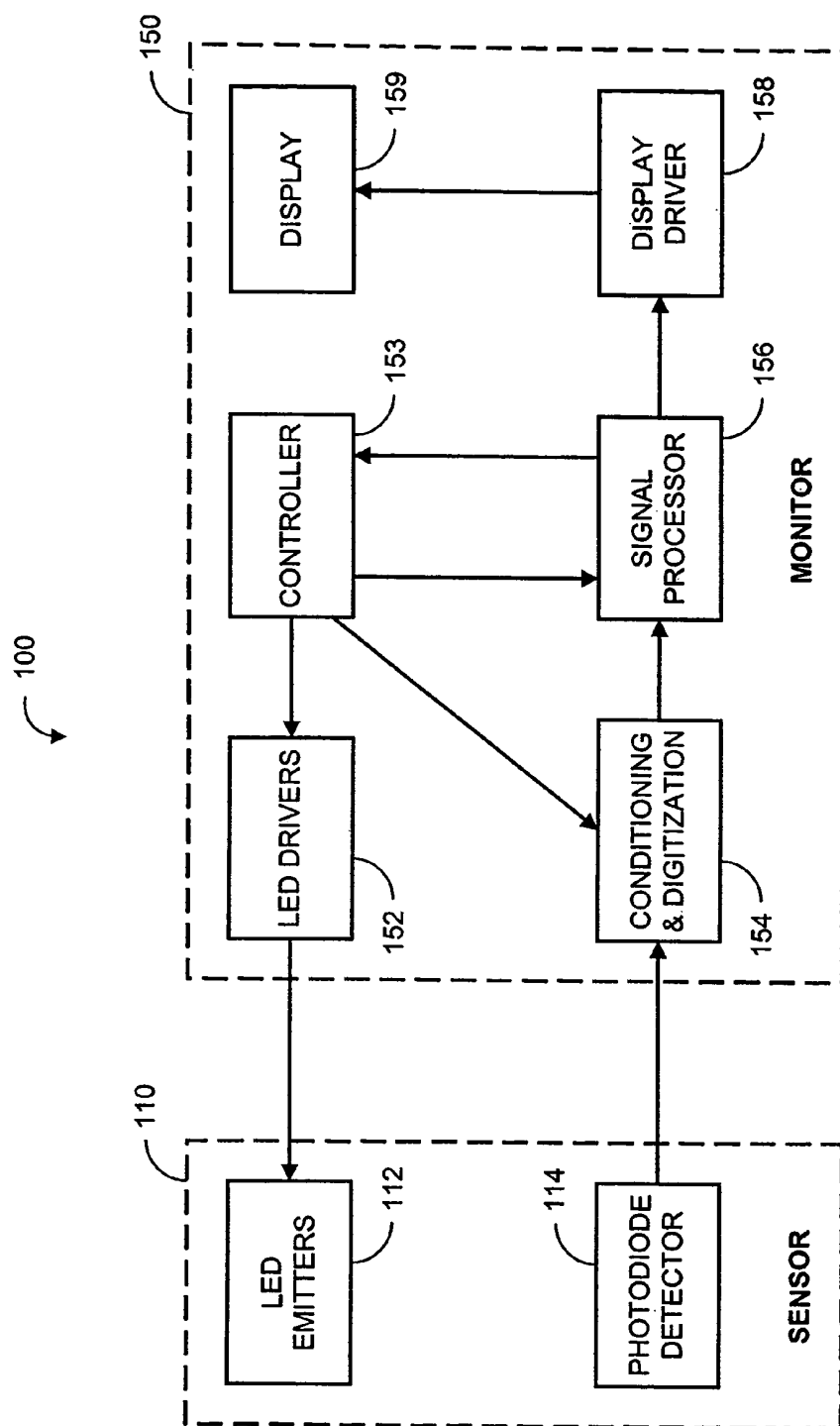


FIG. 1 (Prior Art)

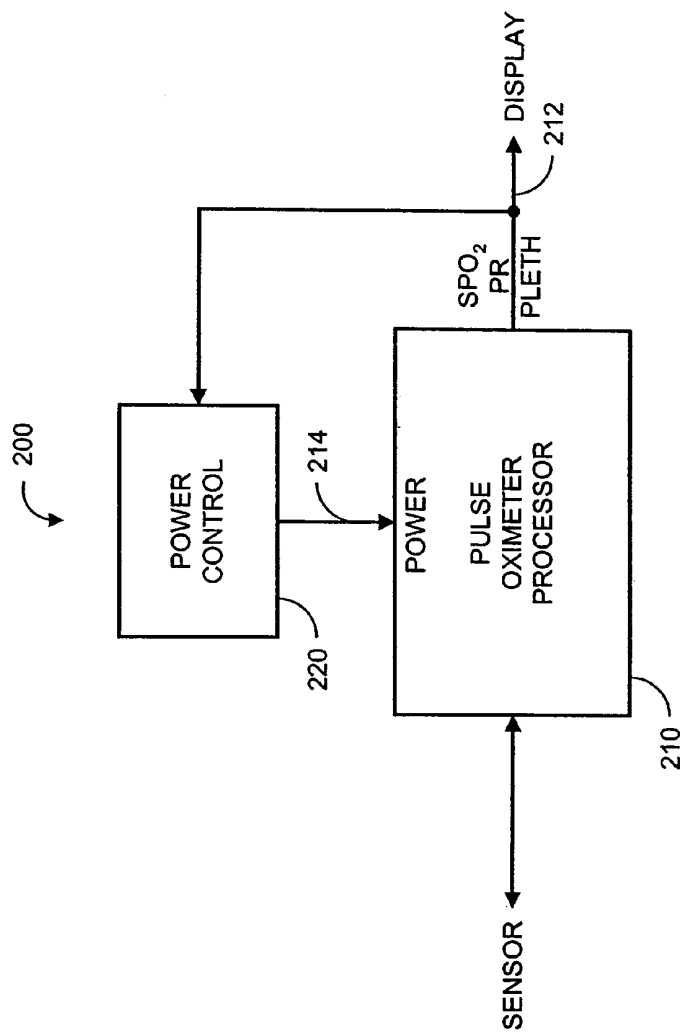


FIG. 2 (Prior Art)

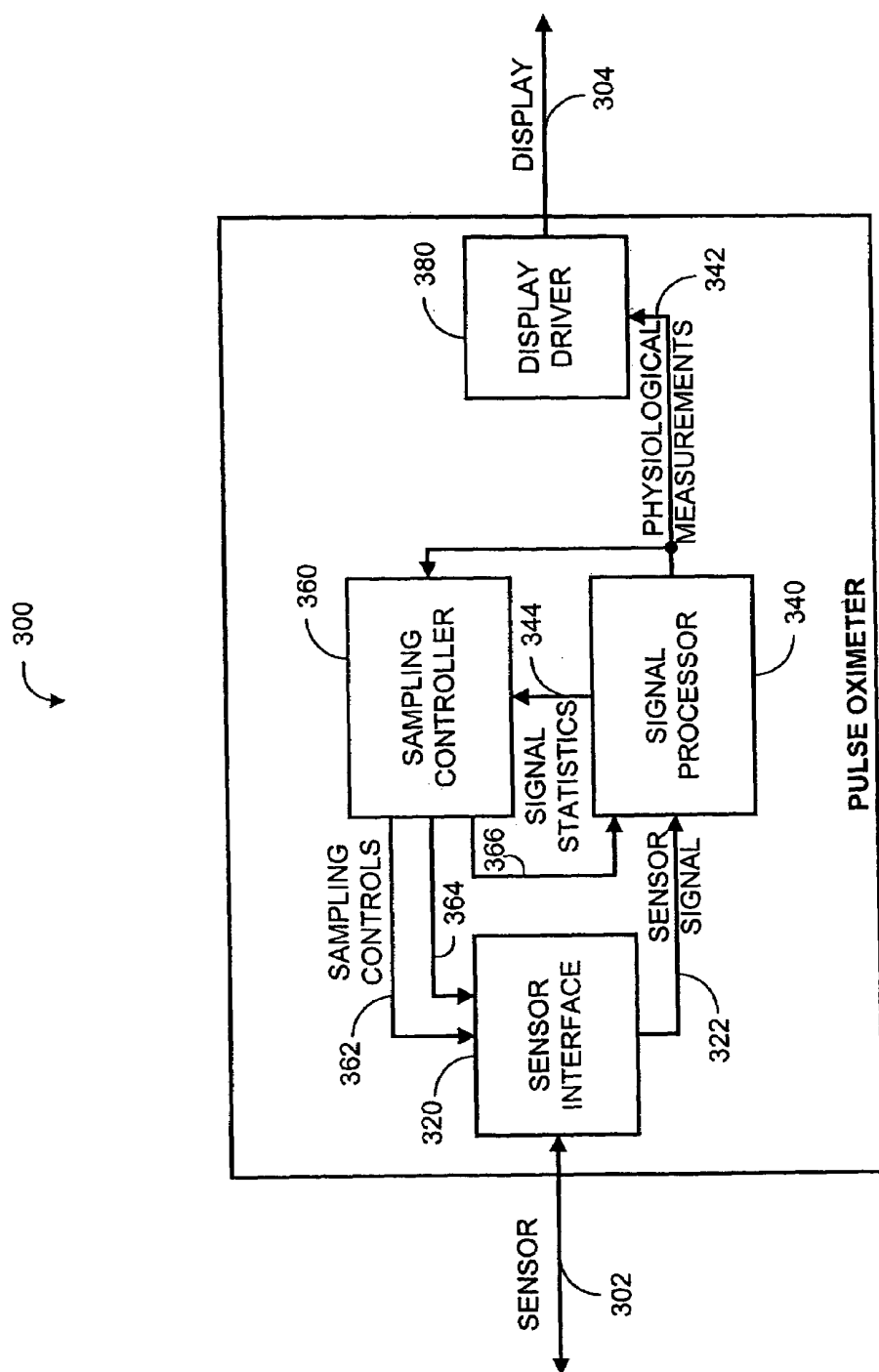


FIG. 3

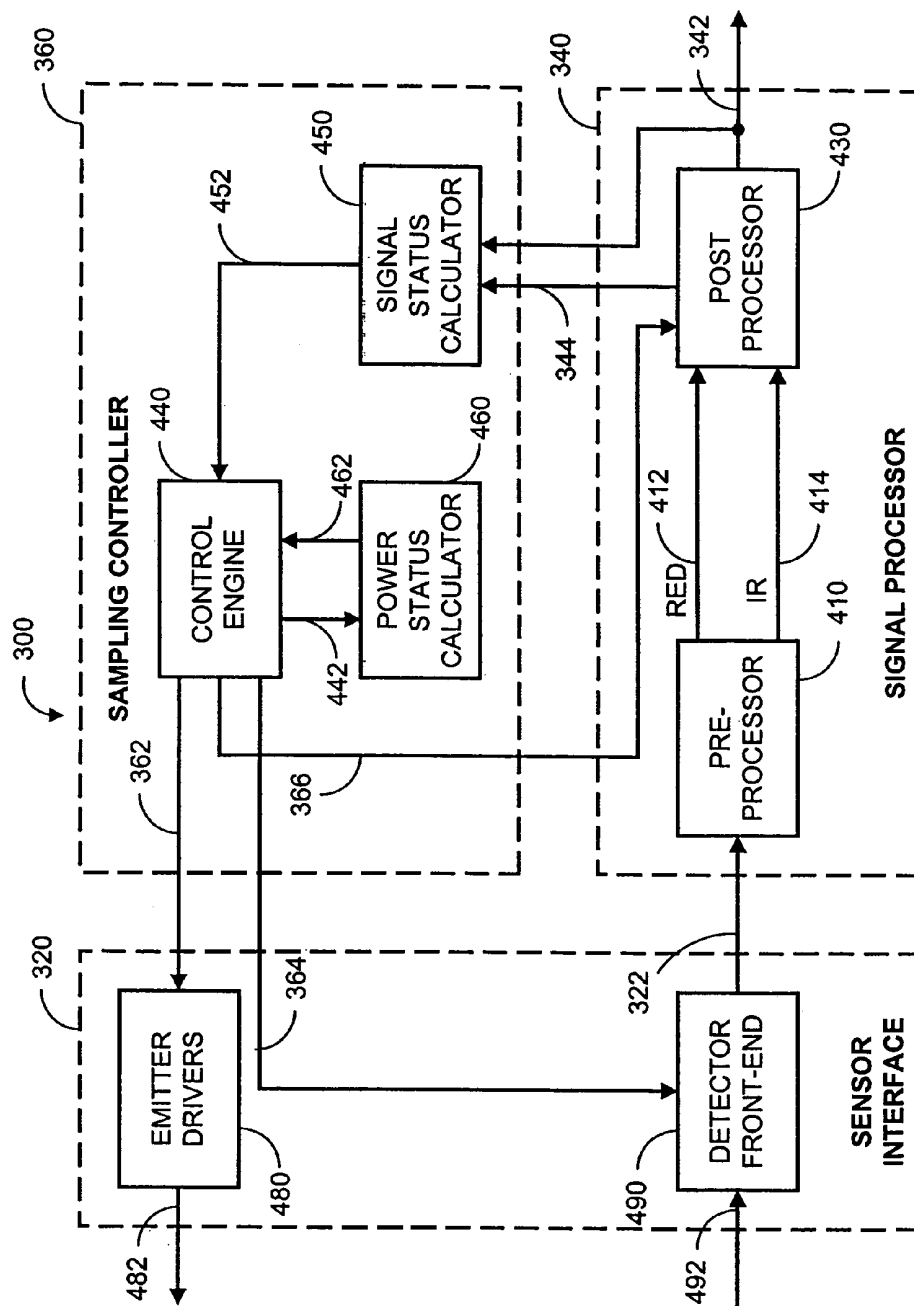


FIG. 4

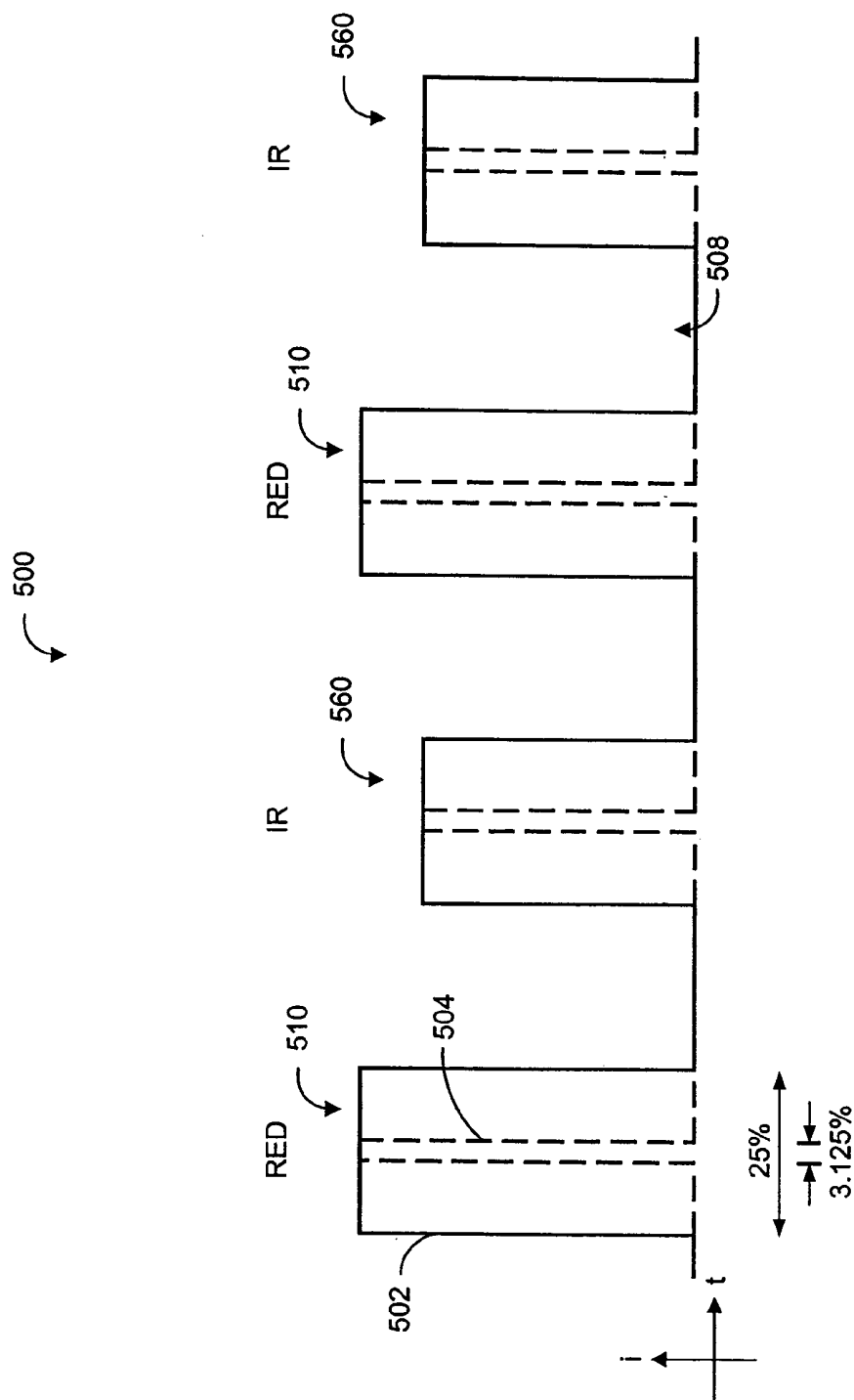


FIG. 5

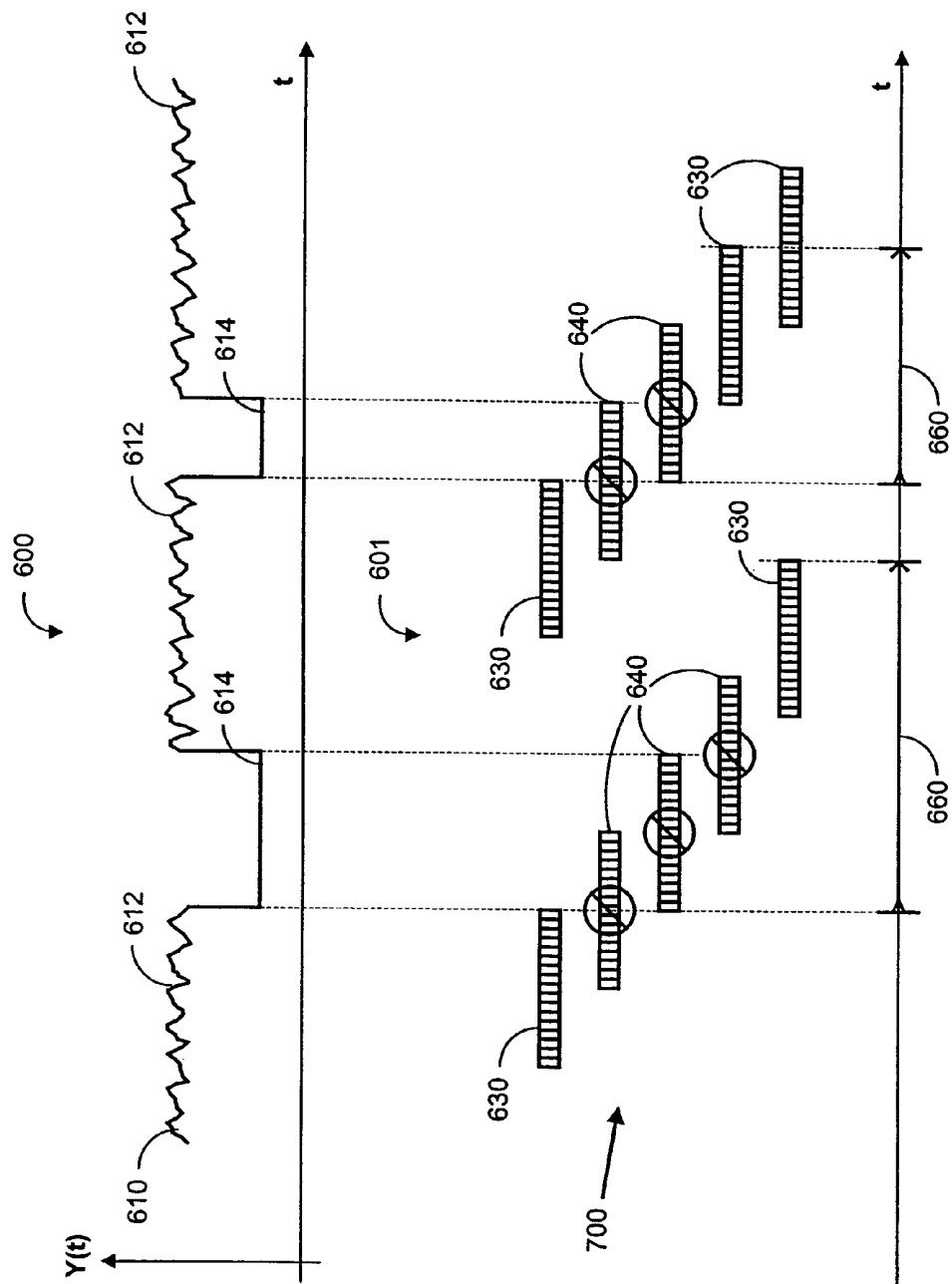


FIG. 6



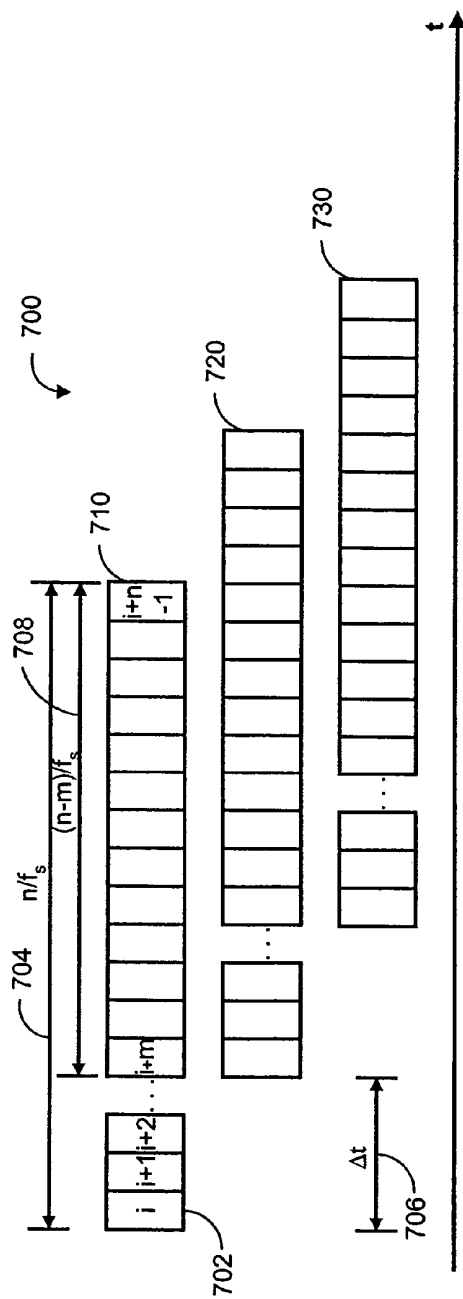


FIG. 7A

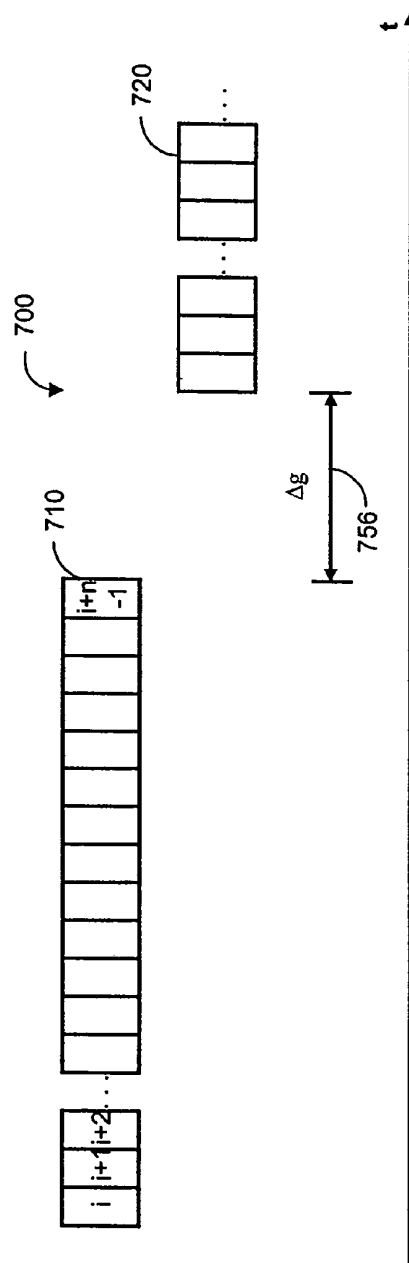


FIG. 7B

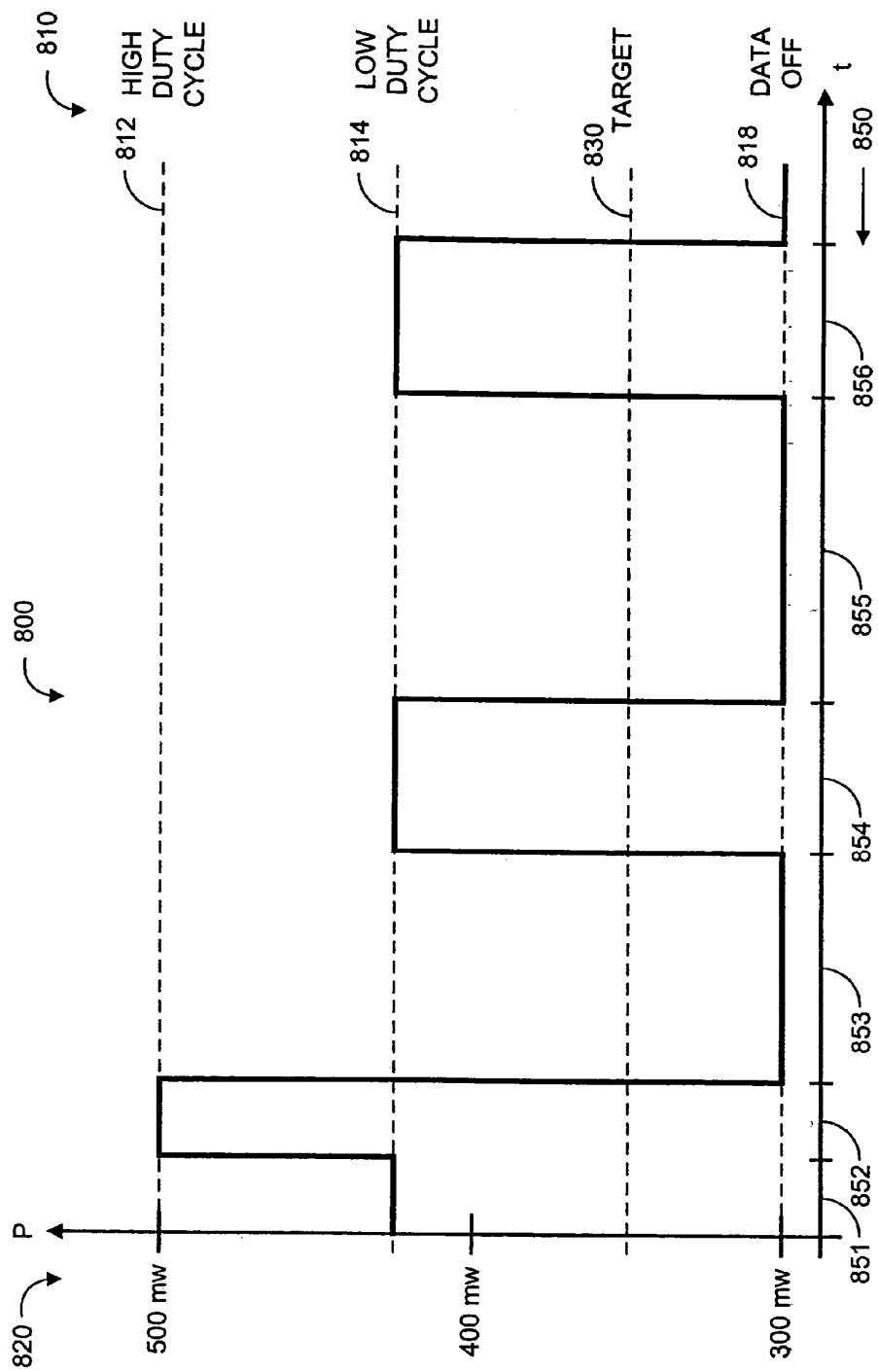


FIG. 8

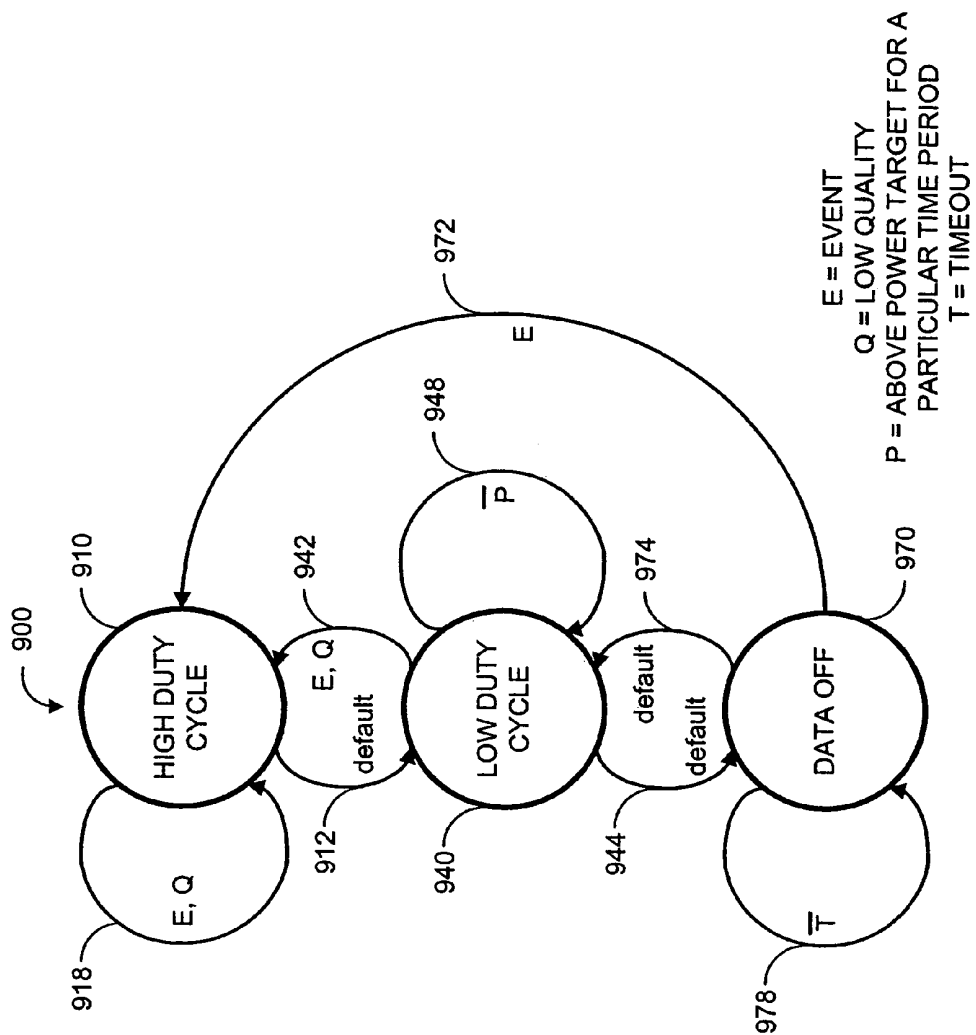


FIG. 9

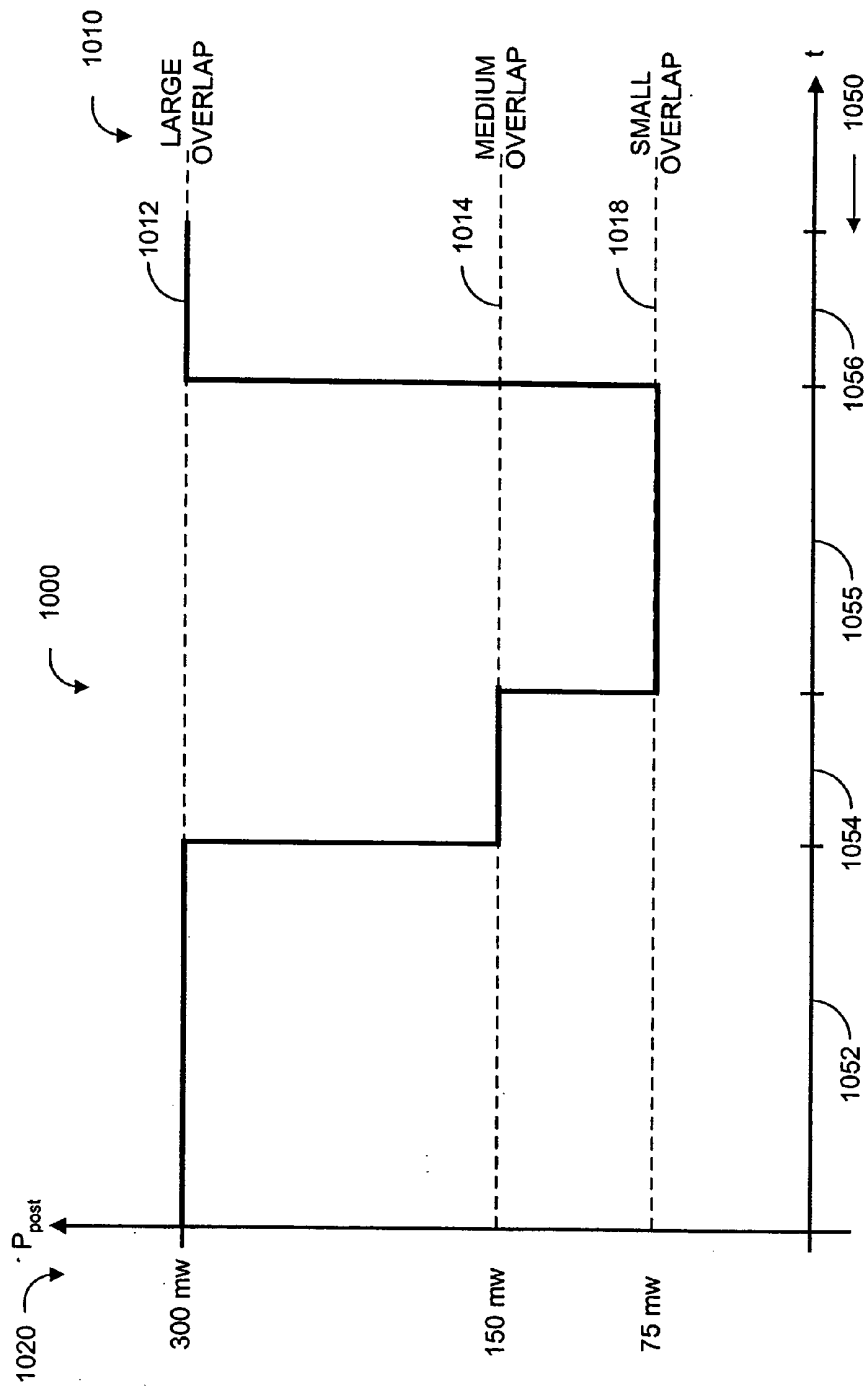


FIG. 10

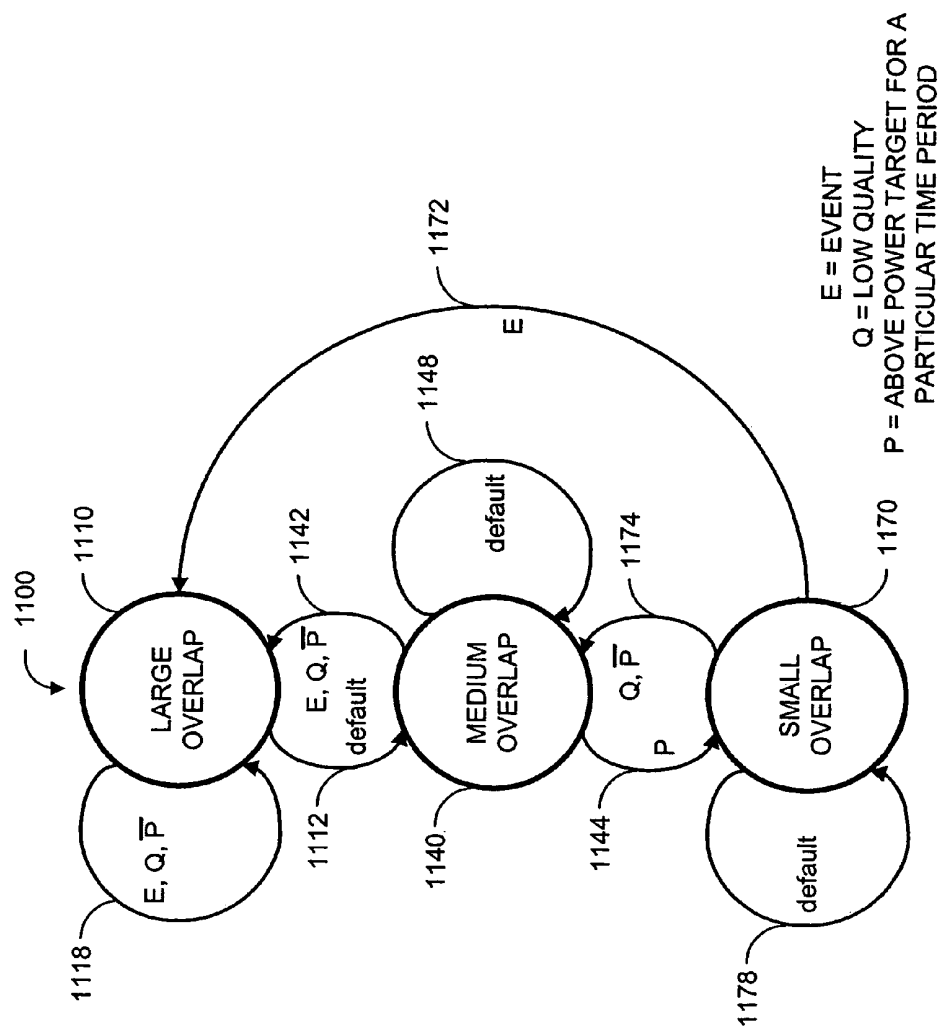


FIG. 11

## LOW POWER PULSE OXIMETER

## REFERENCE TO RELATED APPLICATIONS

The present application claims priority benefit under 35 U.S.C. § 120 to, and is a continuation of application Ser. No. 10/184,028, entitled "Low Power Pulse Oximeter," filed Jun. 26, 2002, now U.S. Pat. No. 6,697,658, which claims priority benefit under 35 U.S.C. § 119(e) from U.S. Provisional Application No. 60/302,564, entitled "Low Power Pulse Oximeter," filed Jul. 2, 2001. The present application incorporates each of the foregoing disclosures herein by reference.

## BACKGROUND OF THE INVENTION

Pulse oximetry is a widely accepted noninvasive procedure for measuring the oxygen saturation level of a person's arterial blood, an indicator of their oxygen supply. Oxygen saturation monitoring is crucial in critical care and surgical applications, where an insufficient blood supply can quickly lead to injury or death. FIG. 1 illustrates a conventional pulse oximetry system 100, which has a sensor 110 and a monitor 150. The sensor 110, which can be attached to an adult's finger or an infant's foot, has both red and infrared LEDs 112 and a photodiode detector 114. For a finger, the sensor is configured so that the LEDs 112 project light through the fingernail and into the blood vessels and capillaries underneath. The photodiode 114 is positioned at the finger tip opposite the fingernail so as to detect the LED emitted light as it emerges from the finger tissues. A pulse oximetry sensor is described in U.S. Pat. No. 6,088,607 entitled "Low Noise Optical Probe," which is assigned to the assignee of the present invention and incorporated by reference herein.

Also shown in FIG. 1, the monitor 150 has LED drivers 152, a signal conditioning and digitization front-end 154, a signal processor 156, a display driver 158 and a display 159. The LED drivers 152 alternately activate the red and IR LEDs 112 and the front-end 154 conditions and digitizes the resulting current generated by the photodiode 114, which is proportional to the intensity of the detected light. The signal processor 156 inputs the conditioned photodiode signal and determines oxygen saturation based on the differential absorption by arterial blood of the two wavelengths emitted by the LEDs 112. Specifically, a ratio of detected red and infrared intensities is calculated by the signal processor 156, and an arterial oxygen saturation value is empirically determined based on the ratio obtained. The display driver 158 and associated display 159 indicate a patient's oxygen saturation, heart rate and plethysmographic waveform.

## SUMMARY OF THE INVENTION

Increasingly, pulse oximeters are being utilized in portable, battery-operated applications. For example, a pulse oximeter may be attached to a patient during emergency transport and remain with the patient as they are moved between hospital wards. Further, pulse oximeters are often implemented as plug-in modules for multiparameter patient monitors having a restricted power budget. These applications and others create an increasing demand for lower power and higher performance pulse oximeters. A conventional approach for reducing power consumption in portable electronics, typically utilized by devices such as calculators and notebook computers, is to have a "sleep mode" where the circuitry is powered-down when the devices are idle.

FIG. 2 illustrates a sleep-mode pulse oximeter 200 utilizing conventional sleep-mode power reduction. The pulse oximeter 200 has a pulse oximeter processor 210 and a power control 220. The power control 220 monitors the pulse oximeter output parameters 212, such as oxygen saturation and pulse rate, and controls the processor power 214 according to measured activity. For example, if there is no significant change in the oxygen saturation value over a certain time period, the power control 220 will power down the processor 210, except perhaps for a portion of memory. The power control 220 may have a timer that triggers the processor 210 to periodically sample the oxygen saturation value, and the power control 220 determines if any changes in this parameter are occurring. If not, the power control 220 will leave the processor 210 in sleep mode.

There are a number of disadvantages to applying consumer electronic sleep mode techniques to pulse oximetry. By definition, the pulse oximeter is not functioning during sleep mode. Unlike consumer electronics, pulse oximetry cannot afford to miss events, such as patient oxygen desaturation. Further, there is a trade-off between shorter but more frequent sleep periods to avoid a missed event and the increased processing overhead to power-up after each sleep period. Also, sleep mode techniques rely only on the output parameters to determine whether the pulse oximeter should be active or in sleep mode. Finally, the caregiver is given no indication of when the pulse oximeter outputs were last updated.

One aspect of a low power pulse oximeter is a sensor interface adapted to drive a pulse oximetry sensor and receive a corresponding input signal. A processor derives a physiological measurement corresponding to the input signal, and a display driver communicates the measurement to a display. A controller generates a sampling control output to at least one of said sensor interface and said processor so as to reduce the average power consumption of the pulse oximeter consistent with a predetermined power target.

In one embodiment, a calculator derives a signal status output responsive to the input signal. The signal status output is communicated to the controller to override the sampling control output. The signal status output may indicate the occurrence of a low signal quality or the occurrence of a physiological event. In another embodiment, the sensor interface has an emitter driver adapted to provide a current output to an emitter portion of the sensor. Here, the sampling control output determines a duty cycle of the current output. In a particular embodiment, the duty cycle may be in the range of about 3.125% to about 25%.

In another embodiment, the sensor interface has a front-end adapted to receive the input signal from a detector portion of the sensor and to provide a corresponding digitized signal. Here, the sampling control output determines a powered-down period of the front-end. A confidence indicator responsive to a duration of the powered-down period may be provided and displayed.

In yet another embodiment, the pulse oximeter comprises a plurality of data blocks responsive to the input signal, wherein the sampling control output determines a time shift of successive ones of the data blocks. The time shift may vary in the range of about 1.2 seconds to about 4.8 seconds.

An aspect of a low power pulse oximetry method comprises the steps of setting a power target and receiving an input signal from a pulse oximetry sensor. Further steps include calculating signal status related to the input signal, calculating power status related to the power target, and sampling based upon the result of the calculating signal status and the calculating power status steps.

In one embodiment, the calculating signal status step comprises the substeps of receiving a signal statistic related to the input signal, receiving a physiological measurement related to the input signal, determining a low signal quality condition from the signal statistic, determining an event occurrence from the physiological measurement, and indicating an override based upon the low signal quality condition or the event occurrence. The calculating power status step may comprise the substeps of estimating an average power consumption for at least a portion of the pulse oximeter, and indicating an above power target condition when the average power consumption is above the power target. The sampling step may comprise the substep of increasing sampling as the result of the override. The sampling step may also comprise the substep of decreasing sampling as the result of the above power target condition, except during the override.

Another aspect of a low power pulse oximetry method comprises the steps of detecting an override related to a measure of signal quality or a physiological measurement event, increasing the pulse oximeter power to a higher power level when the override exists, and reducing the pulse oximeter power to a lower power level when the override does not exist. The method may comprise the further steps of predetermining a target power level for a pulse oximeter and cycling between the lower power level and the higher power level so that an average pulse oximeter power is consistent with the target power level.

In one embodiment, the reducing step comprises the substep of decreasing the duty cycle of an emitter driver output to the sensor. In another embodiment, the reducing step comprises the substep of powering-down a detector front-end. A further step may comprise displaying a confidence indicator related to the duration of the powering-down substep. In yet another embodiment, the reducing step comprises the substep of increasing the time-shift of post-processor data blocks.

Another aspect of a low power pulse oximeter comprises a sensor interface adapted to receive an input signal from a sensor, a signal processor configured to communicate with the sensor interface and to generate an internal parameter responsive to the input signal, and a sampling controller responsive to the internal parameter so as to generate a sampling control to alter the power consumption of at least one of the sensor interface and the signal processor. The signal processor may be configured to generate an output parameter and the sampling controller may be responsive to a combination of the internal and output parameters so as to generate a sampling control to alter the power consumption of at least one of the sensor interface and the signal processor. The internal parameter may be indicative of the quality of the input signal. The output parameter may be indicative of oxygen saturation.

In another embodiment, the sampling controller is responsive to a predetermined power target in combination with the internal parameter so as to generate a sampling control to alter the power consumption of at least one of the sensor interface and the signal processor. The signal processor may be configured to generate an output parameter and the sampling controller may be responsive to a combination of the internal and output parameters and the power target so as to generate a sampling control to alter the power consumption of at least one of the sensor interface and the signal processor. The sensor interface may comprise an emitter driver and the sampling control may modify a duty cycle of the emitter driver. The sensor interface may comprise a detector front-end and the sampling control may intermit-

tently power-down the detector front-end. The processor may generate a plurality of data blocks corresponding to the input signal, where each of the data blocks have a time shift from a preceding one of the data blocks, and where the sampling control may determine the amount of the time shift.

A further aspect of a low power pulse oximeter comprises an interface means for communicating with a sensor, a processor means for generating an internal parameter and an output parameter, and a controller means for selectively reducing the power consumption of at least one of the interface means and the processor means based upon the parameters. In one embodiment, the interface means comprises a driver means for determining the duty cycle of emitter current to the sensor, the driver means being responsive to the controller means. In another embodiment, the interface means comprises a detector front-end means for receiving an input signal from the sensor, the power for the detector front-end means being responsive to the controller means. In yet another embodiment, the processor means comprises a post-processor means for determining a time shift between data blocks, the post-processor means being responsive to the controller means. In a further embodiment, the controller means comprises a signal status calculator means for generating an indication of a low signal quality or a physiological event based upon at least one of an internal signal statistic and an output physiological measurement, and a control engine means in communications with the signal status calculator means for generating a sampling control responsive to the indication. In yet a further embodiment, the controller means comprises a power status calculator means for generating a power indication of power consumption relative to a power target, and a control engine means in communications with the power status calculator means for generating a sampling control responsive to the power indication.

#### BRIEF DESCRIPTION OF THE DRAWINGS

FIG. 1 is a block diagram of a conventional pulse oximeter sensor and monitor;

FIG. 2 is a block diagram of a pulse oximeter having a conventional sleep mode;

FIG. 3 is a top-level block diagram of a low power pulse oximeter;

FIG. 4 is a detailed block diagram of a low power pulse oximeter illustrating a sensor interface, a signal processor and a sampling controller;

FIG. 5 is a graph of emitter drive current versus time illustrating variable duty cycle processing;

FIG. 6 is a graph of oxygen saturation versus time illustrating intermittent sample processing;

FIGS. 7A–B are graphs of data buffer content versus time illustrating variable data block overlap processing;

FIG. 8 is a graph of power versus time illustrating power dissipation conformance to an average power target using variable duty cycle and intermittent sample processing;

FIG. 9 is a state diagram of the sampling controller for variable duty cycle and intermittent sample processing;

FIG. 10 is a graph of power versus time illustrating power dissipation using variable data block overlap processing; and

FIG. 11 is a state diagram of the sampling controller for variable data block overlap processing.

DETAILED DESCRIPTION OF THE  
PREFERRED EMBODIMENT

FIG. 3 illustrates one embodiment of a low power pulse oximeter. The pulse oximeter 300 has a sensor interface 320, a signal processor 340, a sampling controller 360 and a display driver 380. The pulse oximeter 300 also has a sensor port 302 and a display port 304. The sensor port 302 connects to an external sensor, e.g. sensor 110 (FIG. 1). The sensor interface 320 drives the sensor port 302, receives a corresponding input signal from the sensor port 302, and provides a conditioned and digitized sensor signal 322 accordingly. Physiological measurements 342 are input to a display driver 380 that outputs to the display port 304. The display port 304 connects to a display device, such as a CRT or LCD, which a healthcare provider typically uses for monitoring a patient's oxygen saturation, pulse rate and plethysmograph.

As shown in FIG. 3, the signal processor 340 derives the physiological measurements 342, including oxygen saturation, pulse rate and plethysmograph, from the input signal 322. The signal processor 340 also derives signal statistics 344, such as signal strength, noise and motion artifact. The physiological measurements 342 and signal statistics 344 are input to the sampling controller 360, which outputs sampling controls 362, 364, 366 accordingly. The sampling controls 362, 364, 366 regulate pulse oximeter power dissipation by causing the sensor interface 320 to vary the sampling characteristics of the sensor port 302 and by causing the signal processor 340 to vary its sample processing characteristics, as described in further detail with respect to FIG. 4, below. Advantageously, power dissipation is responsive not only to output parameters, such as the physiological measurements 342, but also to internal parameters, such as the signal statistics 344.

FIG. 4 illustrates further detail regarding the sensor interface 320, the signal processor 340 and the sampling controller 360. The sensor interface 320 has emitter drivers 480 and a detector front-end 490. The emitter drivers 480 are responsive to a sampling control 362, described below, and provide emitter drive outputs 482. The emitter drive outputs 482 activate the LEDs of a sensor attached to the sensor port 302 (FIG. 3). The detector front-end 490 receives an input signal 492 from a sensor attached to the sensor port 302 (FIG. 3) and provides a corresponding conditioned and digitized input signal 322 to the signal processor 340. A sampling control 364 controls power to the detector front-end 490, as described below.

As shown in FIG. 4, the signal processor 340 has a pre-processor 410 and a post processor 430. The pre-processor 410 demodulates red and IR signals from the digitized signal 322, performs filtering, and reduces the sample rate. The pre-processor provides a demodulated output, having a red channel 412 and an IR channel 414, which is input into the post-processor 430. The post processor 430 calculates the physiological measurements 342 and the signal statistics 344, which are output to a signal status calculator 450. The physiological measurements 342 are also output to a display driver 380 (FIG. 3) as described above. A pulse oximetry signal processor is described in U.S. Pat. No. 6,081,735 entitled "Signal Processing Apparatus," which is assigned to the assignee of the present invention and incorporated by reference herein.

Also shown in FIG. 4, the sampling controller 360 has a control engine 440, a signal status calculator 450 and a power status calculator 460. The control engine 440 outputs sampling controls 362, 364, 366 to reduce the power con-

sumption of the pulse oximeter 300. In one embodiment, the control engine 440 advantageously utilizes multiple sampling mechanisms to alter power consumption. One sampling mechanism is an emitter duty cycle control 362 that is an input to the emitter drivers 480. The emitter duty cycle control 362 determines the duty cycle of the current supplied by the emitter drive outputs 482 to both red and IR sensor emitters, as described with respect to FIG. 5, below. Another sampling mechanism is a front-end control 364 that intermittently removes power to the detector front-end 490, as described with respect to FIG. 6, below. Yet another sampling mechanism is a data block overlap control 366 that varies the number of data blocks processed by the post processor 430. These various sampling mechanisms provide the flexibility to reduce power without sacrificing performance during, for example, high noise conditions or oxygen desaturation events, as described below in further detail.

The sampling controls 362, 364, 366 modify power consumption by, in effect, increasing or decreasing the number of input samples received and processed. Sampling, including acquiring input signal samples and subsequent sample processing, can be reduced during high signal quality periods and increased during low signal quality periods or when critical measurements are necessary. In this manner, the control engine 440 regulates power consumption to satisfy a predetermined power target, to minimize power consumption, or to simply reduce power consumption, as described with respect to FIGS. 8 and 10, below. The current state of the control engine is provided as a control state output 442 to the power status calculator 460. The control engine 440 utilizes the power status output 462 and the signal status output 452 to determine its next control state, as described with respect to FIGS. 9 and 11, below.

Further shown in FIG. 4, the signal status calculator 450 receives physiological measurements and signal statistics from the post processor 430 and determines the occurrence of an event or a low signal quality condition. An event determination is based upon the physiological measurements output 342 and may be any physiological-related indication that justifies the processing of more sensor samples and an associated higher power consumption level, such as an oxygen desaturation, a fast or irregular pulse rate or an unusual plethysmograph waveform to name a few. A low signal quality condition is based upon the signal statistics output 344 and may be any signal-related indication that justifies the processing of more sensor samples and an associated higher power consumption level, such as a low signal level, a high noise level or motion artifact to name a few. The signal status calculator 450 provides the signal status output 452 that is input to the control engine 440.

In addition, FIG. 4 shows that the power status calculator 460 has a control state input 442 and a power status output 462. The control state input 442 indicates the current state of the control engine 440. The power status calculator 460 utilizes an internal time base, such as a counter, timer or real-time clock, in conjunction with the control engine state to estimate the average power consumption of at least a portion of the pulse oximeter 300. The power status calculator 460 also stores a predetermined power target and compares its power consumption estimate to this target. The power status calculator 460 generates the power status output 462 as an indication that the current average power estimate is above or below the power target and provides this output 462 to the control engine 440.

FIG. 5 illustrates emitter driver output current versus time. The graph 500 depicts the combination of a red LED drive current 510 and an IR drive current 560. The solid line



graph 502 illustrates drive currents having a high duty cycle. The dashed line graph 504 illustrates drive currents having a low duty cycle. In a typical pulse oximeter, the duty cycle of the drive signals is constant and provides sufficient dark bands 508 to demodulate the detector response into red and IR channels. The emitter drivers 480 (FIG. 4), however, require a significant portion of the overall pulse oximeter power budget. Intermittently reducing the drive current duty cycle can advantageously reduce power dissipation without compromising signal integrity. As an example, a low power pulse oximeter implementation nominally consuming 500 mw may be able to reduce power consumption on the order of 70 mw by such drive current duty cycle reductions. In a preferred embodiment, the drive current duty cycle is varied within a range from about 25% to about 3.125%. In a more preferred embodiment, the drive current duty cycle is intermittently reduced from about 25% to about 3.125%. In conjunction with an intermittently reduced duty cycle or as an independent sampling mechanism, there may be a "data off" time period longer than one drive current cycle where the emitter drivers 480 (FIG. 4) are turned off. The detector front-end 490 (FIG. 4) may also be powered down during such a data off period, as described with respect to FIGS. 8 and 9, below.

FIG. 6 is a graph 600 of a pre-processor output signal 610 over time depicting the result of intermittent sampling at the detector front-end 490 (FIG. 4). The output signal 610 is a red channel 412 (FIG. 4) or an IR channel 414 (FIG. 4) output from the pre-processor 410 (FIG. 4), which is input to the post processor 430 (FIG. 4), as described above. The output signal 610 has "on" periods 612, during which time the detector front-end 490 (FIG. 4) is powered-up and "off" periods 614, during which time the detector front-end 490 (FIG. 4) is powered-down. The location and duration of the on periods 612 and off periods 614 are determined by the front-end control 364 (FIG. 4).

Also shown in FIG. 6 is a corresponding timeline 601 of overlapping data blocks 700, which are "snap-shots" of the pre-processor output signal 610 over specific time intervals. Specifically, the post processor 430 (FIG. 4) processes a sliding window of samples of the pre-processor output signal 610, as described with respect to FIGS. 7A-B, below. Advantageously, the post processor 430 (FIG. 4) continues to function during off portions 614, marking as invalid those data blocks 640 that incorporate off portions 614. A freshness counter can be used to measure the time period 660 between valid data blocks 630, which can be displayed on a pulse oximeter monitor as an indication of confidence in the current measurements.

FIGS. 7A-B illustrate data blocks 700, which are processed by the post processor 430 (FIG. 4). Each data block 700 has  $n$  samples 702 of the pre-processor output and corresponds to a time interval 704 of  $n/f_s$ , where  $f_s$  is the sample frequency. For example, in one embodiment  $n=600$  and  $f_s=62.5$  Hz. Hence, each data block time interval 704 is nominally 9.6 sec.

As shown in FIG. 7A, each data block 700 also has a relative time shift 706 from the preceding data block, where is an integral number of sample periods. That is,  $=m/f_s$ , where  $m$  is an integer representing the number of samples dropped from the preceding data block and added to the succeeding data block. In the embodiment described above,  $m=75$  and  $=1.2$  sec, nominally. The corresponding overlap 708 of two adjacent data blocks 710, 720 is  $(n-m)/f_s$ . In the embodiment described above, the overlap 708 is nominally 9.6 sec-1.2 sec=8.4 sec. The greater the overlap 708, i.e. the smaller the time shift 706, the more data blocks there are to

process in the post-processor 430 (FIG. 4), with a corresponding greater power consumption. The overlap 708 between successive data blocks 710, 720 may vary from  $n-1$  samples to no samples, i.e. no overlap. Also, as shown in FIG. 7B, there may be a sample gap 756 or negative overlap, i.e. samples between data blocks that are not processed by the post-processor, allowing further post-processor power savings. Sample gaps 756 may correspond to detector front-end off periods 614 (FIG. 6).

FIG. 8 illustrates an exemplar power consumption versus time profile 800 for the pulse oximeter 300 (FIG. 3) during various control engine states. In one embodiment, the control engine 440 (FIG. 4) has three states related to the sampling control outputs 362, 364 that affect pulse oximeter power consumption accordingly. One of ordinary skill in the art will recognize that the control engine 440 (FIG. 4) may have greater or fewer states and associated power consumption levels. The profile 800 shows the three control engine states 810 and the associated power consumption levels 820. These three states are high duty cycle 812, low duty cycle 814 and data off 818.

In the high duty cycle state 812, the control engine 440 (FIG. 4) causes the emitter drivers 480 (FIG. 4) to turn on sensor emitters for a relatively long time period, such as 25% on time for each of the red 510 and IR 560 drive currents. In the low duty cycle state 814, the control engine 440 (FIG. 4) causes the emitter drivers 480 (FIG. 4) to turn on sensor emitters for a relatively short time period, such as 3.125% of the time for each of the red 510 and IR 560 drive currents. In the data off state 818, the control engine 440 (FIG. 4) turns off the emitter drivers 480 (FIG. 4) and powers down the detector front-end 490 (FIG. 4). Also shown is a predetermined target power consumption level 830. The control engine 440 (FIG. 4) alters the sensor sampling of the pulse oximeter 300 (FIG. 3) so that the average power consumption matches the target level 830, as indicated by the power status output 462 (FIG. 4), except when overridden by the signal status output 452 (FIG. 4).

As shown in FIG. 8, power consumption changes according to the control states 810 during each of the time intervals 850. In a first time interval 851, the pulse oximeter is in a low duty cycle state 814 and transitions to a high duty cycle state 812 during a second time interval 852 due to an event or low quality signal. During a third time interval 853, the pulse oximeter is able to enter the data off state 818, during which time no sensor samples are processed. In a fourth time interval 854, sensor samples are again taken, but at a low duty cycle 814. During the fifth and sixth time intervals 855, 856, sensor samples are shut off and turned on again as the pulse oximeter 300 (FIG. 3) alternates between the data off state 818 and the low duty cycle state 814 so as to maintain an average power consumption at the target level 830.

FIG. 9 illustrates a state diagram 900 for one embodiment of the control engine 440 (FIG. 4). In this embodiment, there are three control states, high duty cycle 910, low duty cycle 940 and data off 970, as described with respect to FIG. 8, above. If the control state is data off 970, an event triggers a data-off to high-duty-cycle transition 972. If the control state is low duty cycle 940, an event similarly triggers a low-duty cycle to high-duty-cycle transition 942. In this manner, the occurrence of an event initiates high duty sensor sampling, allowing high fidelity monitoring of the event. Similarly, if the control state is low duty cycle 940, low signal quality triggers a low-duty cycle to high-duty-cycle transition 942. In this manner, low signal quality initiates higher duty sensor sampling, providing, for example, a larger signal-to-noise ratio.

Also shown in FIG. 9, if the control state is high duty cycle **910** and either an event is occurring or signal quality is low, then a null transition **918** maintains the high duty cycle state **910**. If the pulse oximeter is not above the power target for more than a particular time interval, a null transition **948** maintains the low duty cycle state **940**, so that sampling is turned-off only when necessary to track the power target. Further, if the control state is data off **970** and no time-out has occurred, a null transition **978** maintains the data off state **970**, providing a minimum power consumption.

In addition, FIG. 9 shows that when the control state is in a high duty cycle state **910**, if neither an event nor low signal quality are occurring, then a high-duty-cycle to low-duty-cycle transition **912** occurs by default. Also, if the control state is low duty cycle **940**, if neither an event nor low signal quality are occurring and the power consumption is above the target level for longer than a particular time interval, a low-duty-cycle to data-off transition **944** occurs by default, allowing power consumption to come down to the target level. Further, if the control state is data off **970**, if no event occurs and a timeout does occur, a data-off to low-duty-cycle transition **974** occurs by default, preventing excessively long periods of no sensor sampling.

FIG. 10 illustrates an exemplar power consumption versus time profile **1000** for the post processor **430** (FIG. 4) during various control engine states. In one embodiment, the control engine **440** (FIG. 4) has three states related to the sampling control output **366** (FIG. 4) that affect post processor power consumption accordingly. One of ordinary skill in the art will recognize that the control engine may have greater or fewer states and associated power consumption levels. The profile **1000** shows the three control engine states **1010** and the associated post processor power consumption levels **1020**. These three states are large overlap **1012**, medium overlap **1014** and small overlap **1018**.

As shown in FIG. 10, in the large overlap state **1012**, the control engine **440** (FIG. 4) causes the post processor to process data blocks that have a comparatively small time shift **706** (FIG. 7A), and the post processor exhibits relatively high power consumption under these conditions, say 300 mw. In the medium overlap state **1014**, the control engine **440** (FIG. 4) causes the post processor to process data blocks that have a comparatively larger time shift **706** (FIG. 7A). For example, the data blocks may be time shifted twice as much as for the large overlap state **1012**, and, as such, the post processor performs only half as many computations and consumes half the nominal power, say 150 mw. In the small overlap state **1018**, the control engine **440** (FIG. 4) causes the post processor to process data blocks that have a comparatively large time shift. For example, the data blocks may be time shifted twice as much as for the medium overlap state **1014**. As such, the post processor performs only a quarter as many computations and consumes a quarter of the nominal power, say 75 mw, as for the large overlap state **1012**. In one embodiment, the control engine **440** (FIG. 4) alters the data block overlap of the post processor in conjunction with the duty cycle of the emitter drivers described with respect to FIG. 5, above, and the front-end sampling described with respect to FIG. 6, above, so that the average power consumption of the pulse oximeter matches a target level indicated by the power status output **462** (FIG. 4) or so that the power consumption is otherwise reduced or minimized.

In a preferred embodiment, data blocks are time shifted by either about 0.4 sec or about 1.2 sec, depending on the overlap state of the control engine **440** (FIG. 4). In a more

preferred embodiment, the data blocks are varied between about 1.2 sec and about 4.8 sec. In a most preferred embodiment, the data blocks are time shifted by either about 1.2 sec, about 2.4 sec or about 4.8 sec, depending on the overlap state of the control engine **440** (FIG. 4). Although the post-processing of data blocks is described above with respect to only a few overlap states and a corresponding number of particular data block time shifts, there may be many overlap states and a corresponding range of data block time shifts.

Further shown in FIG. 10, power consumption **1020** changes according to the control states **1010** during each of the time intervals **1050**. In a first time interval **1052**, the post processor is in a large overlap state **1012** and transitions to a medium overlap state **1014** during a second time interval **1054**, so as to meet a power target during a high signal quality period, for example. During a third time interval **1055**, the post processor enters a small overlap state **1018**, for example to meet a power target by further reducing power consumption. In a forth time interval **1056**, the post processor transitions back to a large overlap state **1012**, such as during an event or low signal quality conditions.

FIG. 11 illustrates a state diagram **1100** for one embodiment of the control engine **440** (FIG. 4). These states may function in parallel with, or in combination with, the sampling states described with respect to FIG. 9, above. In the illustrated embodiment, there are three control states, large overlap **1110**, medium overlap **1140** and small overlap **1170**, as described with respect to FIG. 10, above. If the control state is small overlap **1170**, an event triggers a small overlap to large overlap transition **1172**. If the control state is medium overlap **1140**, an event similarly triggers a medium overlap to large-overlap transition **1142**. In this manner, the occurrence of an event initiates the processing of more data blocks, allowing more robust signal statistics and higher fidelity monitoring of the event. Similarly, if the control state is medium overlap **1140**, low signal quality triggers a medium overlap to large overlap transition **1142**. In this manner, low signal quality initiates the processing of more data blocks, providing more robust signal statistics during lower signal-to-noise ratio periods.

Also shown in FIG. 11, if the control state is large overlap **1110** and either an event is occurring or signal quality is low, then a null transition **1118** maintains the large overlap state **1110**. If the pulse oximeter is not above the power target for more than a particular time interval, a null transition **1148** maintains the medium overlap state **1140**, so that reduced data processing occurs only when necessary to track the power target. Further, if the control state is small overlap **1170**, a null transition **1178** maintains this power saving state until the power target is reached or an event or low signal quality condition occurs.

In addition, FIG. 11 shows that when the control state is in a large overlap state **1110**, if neither an event nor low signal quality are occurring, then a large overlap to medium overlap transition **1112** occurs by default. Also, if the control state is medium overlap **1140**, if the power consumption is above the target level for longer than a particular time interval and no low signal quality condition or event is occurring, a medium overlap to small overlap transition **1174** occurs, allowing power consumption to come down to the target level. Further, if the control state is small overlap **1170**, if no event occurs but the power target has been met, a small overlap to medium overlap transition **1174** occurs.

A low power pulse oximeter embodiment is described above as having a power status calculator **460** (FIG. 4) and an associated power target. Another embodiment of a low

power pulse oximeter, however, functions without either a power status calculator or a power target, utilizing the sampling controls 362, 364, 366 (FIG. 3) in response to internal parameters and/or output parameters, such as signal statistics 344 (FIG. 3) and/or physiological measurements 342 (FIG. 3) to reduce power consumption except during, say, periods of low signal quality and physiological events.

One of ordinary skill in the art will recognize that various state diagrams are possible representing control of the emitter drivers, the detector front-end and the post-processor. Such state diagrams may have fewer or greater states with differing transitional characteristics and with differing relationships between sampling mechanisms than the particular embodiments described above. In relatively simple embodiments of the control engine 440 (FIG. 4), only a single sampling mechanism is used, such as the sampling mechanism used to vary the duty cycle of the emitter drivers. The single sampling mechanism may be based only upon internal parameters, such as signal quality, only upon output parameters, such as those that indicate the occurrence of physiological events, or upon a combination of internal and output parameters, with or without a power target.

In relatively more complex embodiments of the control engine 440 (FIG. 4), sampling mechanisms are used in combination. These sampling mechanisms may be based only upon internal parameters, only upon output parameters, or upon a combination of internal and output parameters, with or without a power target. In a particular embodiment, the emitter duty-cycle, front-end duty-cycle and data block overlap sampling mechanisms described above are combined. A “reduced overlap” state relating to the post-processing of data blocks is added to the diagram of FIG. 9 between the “low duty cycle” state and the “data off” state. That is, sampling is varied between a high duty cycle state, a low duty cycle state, a reduced overlap state and a data off state in response to signal quality and physiological events, with or without a power target.

The low power pulse oximeter has been disclosed in detail in connection with various embodiments. These embodiments are disclosed by way of examples only and are not to limit the scope of the claims that follow. One of ordinary skill in the art will appreciate many variations and modifications.

What is claimed is:

1. A method of managing power consumption in a pulse oximeter, the method comprising:

operating a pulse oximeter at a first approximate power consumption during a first signal condition representative of a condition of a signal received from a sensor capable of detecting energy attenuated by tissue of a measurement site of a patient;

determining a second signal condition of the signal; and operating the pulse oximeter at a second approximate power consumption different than the first approximate power consumption based on the second signal condition, wherein the step of operating the pulse oximeter at the first approximate power consumption comprises generating a drive signal for the sensor at a first duty cycle, and wherein the step of operating the pulse oximeter at the second approximate power consumption comprises generating the drive signal for the sensor at a second duty cycle different from the first duty cycle.

2. The method of claim 1, wherein the first signal condition corresponds to a high signal quality condition and the first approximate power consumption corresponds to a low power consumption.

3. The method of claim 1, wherein the second signal condition corresponds to a low signal quality condition and the second approximate power consumption corresponds to a high power consumption.

4. The method of claim 1, wherein the first duty cycle comprises approximately three percent (3%) and the second duty cycle comprises approximately twenty-five percent (25%).

5. The method of claim 1, wherein the steps of operating the pulse oximeter at a first approximate power consumption and operating the pulse oximeter at a second approximate power consumption comprises varying a duty cycle of a drive signal for the sensor.

6. The method of claim 5, wherein the varying the duty cycle comprises varying the duty cycle between approximately three percent (3%) and approximately twenty-five percent (25%).

7. The method of claim 1 wherein the steps of operating the pulse oximeter at the first approximate power consumption and of operating the pulse oximeter at the second approximate power consumption comprises varying an amount of data blocks processed.

8. The method of claim 1, wherein the steps of operating the pulse oximeter at the first approximate power consumption and of operating the pulse oximeter at the second approximate power consumption comprises varying power to a detector front end.

9. The method of claim 1, comprising:

determining an override condition exists; and

returning to operating the pulse oximeter at the first approximate power consumption.

10. A pulse oximeter capable of varying its power consumption, comprising:

an emitter driver which outputs a drive signal capable of driving at least one emitter of a sensor that detects energy attenuated by tissue of a measurement site of a patient; and

a controller which selects between at least a first duty cycle of the drive signal corresponding to a first power consumption and a second duty cycle of the drive signal corresponding to a second power consumption different than the first power consumption.

11. The pulse oximeter of claim 10, wherein the first power consumption corresponds to a low power consumption and is associated with a high signal quality of at least one signal received from the sensor.

12. The pulse oximeter of claim 10, wherein second power consumption corresponds to a high power consumption and is associated with a low signal quality of at least one signal received from the sensor.

13. The pulse oximeter of claim 10, wherein the first duty cycle is substantially lower than the second duty cycle.

14. The pulse oximeter of claim 13, wherein the first duty cycle comprises approximately three percent (3%) and the second duty cycle comprises approximately twenty-five percent (25%).

15. The pulse oximeter of claim 10, wherein the controller varies an amount of data blocks processed.

16. The pulse oximeter of claim 10, wherein the controller varies power to a detector front end.

17. The pulse oximeter of claim 10, wherein the controller selects based on at least an estimate of power consumption as compared to a target power consumption.

18. The pulse oximeter of claim 10, wherein the controller selects based on a quality of a signal responsive to the detected energy from said sensor.

13

19. The pulse oximeter of claim 10, wherein the controller selects based on one or more determined values of a physiological parameter responsive to the detected energy from said sensor.

20. A method of modifying power consumption of an oximeter, the method comprising:

operating said oximeter at a lower power consumption by at least one of activating emitters of a noninvasive optical sensor at a decreased duty cycle or reducing overlap in data blocks being processed;

determining a transition event should occur; and

operating said oximeter at a higher power consumption based at least in part on said determination of said transition event by at least one of activating said emitters of said sensor at an increased duty cycle or increasing overlap in said data blocks being processed.

21. The method of claim 20, wherein the operating said oximeter at said lower power consumption comprises activating said emitters at said decreased duty cycle, and wherein the operating said oximeter at said higher power consumption comprises activating said emitters at said increased duty cycle.

22. The method of claim 21, wherein said decreased duty cycle can range as low as about 3.125% and said increased duty cycle can range as high as about 25%.

23. The method of claim 20, wherein the operating said oximeter at said lower power consumption comprises decreasing said overlap, and wherein the operating said oximeter at said higher power consumption comprises increasing said overlap.

24. The method of claim 23, wherein said decreased overlap is associated with a time shift ranging as high as about 4.8 seconds and said increased overlap is associated with a time shift ranging as low as about 1.2 seconds.

14

25. The method of claim 20, wherein the operating said oximeter at said lower power consumption additionally comprises intermittently removing power from a processing front end, and wherein the operating said oximeter at said higher power consumption additionally comprises powering said processing front end.

26. The method of claim 20, wherein said determining said transition event should occur comprises evaluating one or more characteristics of one or more signals from one or more light sensitive detectors.

27. The method of claim 26, wherein said one or more characteristics comprises signal strength.

28. The method of claim 26, wherein said one or more characteristics comprises a presence of noise.

29. The method of claim 26, wherein said one or more characteristics comprises a presence of motion induced noise.

30. The method of claim 20, wherein said determining said transition event should occur comprises determining an estimate of current power consumption and comparing said estimate with a target power consumption.

31. The method of claim 20, wherein said determining said transition event should occur comprises determining an override condition exists.

32. The method of claim 31, wherein said override condition comprises a need for measurements during a critical care environment.

33. The method of claim 31, wherein said override condition comprises one or more monitored physiological parameters exhibiting predefined behavior.

\* \* \* \* \*

UNITED STATES PATENT AND TRADEMARK OFFICE  
**CERTIFICATE OF CORRECTION**

PATENT NO. : 7,295,866 B2  
APPLICATION NO. : 10/785573  
DATED : November 13, 2007  
INVENTOR(S) : Ammar Al-Ali

Page 1 of 1

It is certified that error appears in the above-identified patent and that said Letters Patent is hereby corrected as shown below:

At column 12, line 14, in claim 6, after “wherein”, please delete “the”.

At column 12, line 18, in claim 7, after “claim 1”, please insert -- , --.

Signed and Sealed this

Eighteenth Day of November, 2008

A handwritten signature in black ink, reading "Jon W. Dudas". The signature is stylized, with a large, looped initial "J" and a distinct "D" at the end.

JON W. DUDAS  
*Director of the United States Patent and Trademark Office*

专利名称(译)	低功耗脉搏血氧仪		
公开(公告)号	<a href="#">US7295866</a>	公开(公告)日	2007-11-13
申请号	US10/785573	申请日	2004-02-24
[标]申请(专利权)人(译)	AL ALI AMMAR		
申请(专利权)人(译)	AL-ALI AMMAR		
当前申请(专利权)人(译)	Masimo公司		
[标]发明人	AL ALI AMMAR		
发明人	AL-ALI, AMMAR		
IPC分类号	A61B5/00		
CPC分类号	A61B5/1455 A61B5/14551 A61B2560/0209		
优先权	60/302564 2001-07-02 US		
其他公开文献	US20040181133A1		
外部链接	<a href="#">Espacenet</a> <a href="#">USPTO</a>		

#### 摘要(译)

脉冲血氧计自适应地对来自传感器的输入信号进行采样，以便在没有超控条件的情况下降低功耗。各种采样机制可以单独使用或组合使用，包括减小驱动电流到传感器发射器的占空比，间歇地将前端接口断电到传感器检测器，或者增加处理数据块之间的时移。可以监视内部参数和输出参数以触发或覆盖降低的功耗状态。以这种方式，脉冲血氧计可以在例如高噪声条件或氧饱和度降低期间降低功耗而不牺牲性能。

