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(54) **SYSTEM AND METHOD FOR A SELF-CALIBRATING NON-INVASIVE SENSOR**

(75) Inventor: **Thomas Dietiker**, Rancho Palos Verdes, CA (US)

(73) Assignee: **Elekon Industries USA, Inc.**, Torrance, CA (US)

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G01D 18/00 (2006.01)

(52) **U.S. Cl.** **702/104**; 702/85; 356/40; 600/310; 600/331; 600/473; 600/476

(58) **Field of Classification Search** 702/104, 702/85, 196; 356/40; 600/320, 328, 323, 600/473, 476, 310, 331

See application file for complete search history.

(56) **References Cited**

U.S. PATENT DOCUMENTS

- 3,638,640 A 2/1972 Shaw
- 3,799,672 A 3/1974 Vurek
- 3,998,550 A 12/1976 Konishi et al.

- 4,603,700 A 8/1986 Nichols et al.
- 4,621,643 A 11/1986 New, Jr. et al.
- 4,653,498 A 3/1987 New, Jr. et al.
- 4,700,708 A 10/1987 New, Jr. et al.
- 4,714,080 A 12/1987 Edgar, Jr. et al.
- 4,770,179 A 9/1988 New, Jr. et al.
- 4,796,636 A 1/1989 Branstetter et al.
- 4,824,242 A 4/1989 Frick et al.
- 4,834,532 A 5/1989 Yount
- 4,867,557 A 9/1989 Takatani et al.
- 4,869,253 A 9/1989 Craig, Jr. et al.
- 4,913,150 A 4/1990 Cheung et al.
- 4,942,877 A 7/1990 Sakai et al.
- 5,058,588 A 10/1991 Kaestle
- 5,111,817 A 5/1992 Clark et al.
- 5,190,038 A 3/1993 Polson et al.
- 5,216,598 A 6/1993 Branstetter et al.
- 5,218,962 A 6/1993 Mannheimer et al.
- 5,246,002 A 9/1993 Prosser

(Continued)

FOREIGN PATENT DOCUMENTS

EP 0 898 932 A1 3/1999

(Continued)

OTHER PUBLICATIONS

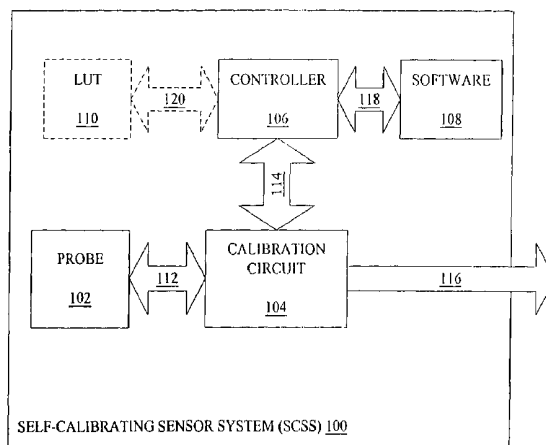
PCT International Search Report; Dated Feb. 27, 2002.

Primary Examiner—John Barlow
Assistant Examiner—Hien Vo
(74) *Attorney, Agent, or Firm*—Factor & Lake

(57) **ABSTRACT**

A non-invasive emitter-photodiode sensor which is able to provide a data-stream corresponding to the actual wavelength of light emitted thereby allowing calibration of the sensor signal processing equipment and resulting in accurate measurements over a wider variation in emitter wavelength ranges.

20 Claims, 13 Drawing Sheets



U.S. PATENT DOCUMENTS

5,259,381 A 11/1993 Cheung et al.
 5,267,562 A 12/1993 Ukawa et al.
 5,278,627 A 1/1994 Aoyagi et al.
 5,279,295 A 1/1994 Martens et al.
 5,368,224 A 11/1994 Richardson et al.
 5,377,674 A 1/1995 Kuestner
 5,398,680 A 3/1995 Polson et al.
 5,421,329 A 6/1995 Casciani et al.
 5,448,991 A 9/1995 Polson et al.
 5,490,505 A 2/1996 Diab et al.
 5,503,148 A 4/1996 Pologe et al.
 5,564,417 A 10/1996 Chance
 5,632,272 A 5/1997 Diab et al.
 5,645,059 A 7/1997 Fein et al.
 5,685,299 A 11/1997 Diab et al.
 5,692,505 A 12/1997 Fouts
 5,694,930 A 12/1997 Pries et al.
 5,758,644 A 6/1998 Diab et al.
 5,779,630 A 7/1998 Fein et al.
 5,782,756 A 7/1998 Mannheimer
 5,807,247 A 9/1998 Merchant et al.
 5,820,550 A 10/1998 Polson et al.
 5,823,950 A 10/1998 Diab et al.
 5,827,182 A 10/1998 Raley et al.
 5,830,137 A 11/1998 Scharf
 5,841,536 A 11/1998 Dimmick
 5,842,981 A 12/1998 Larsen et al.
 5,921,921 A 7/1999 Potratz et al.
 5,934,277 A 8/1999 Mortz
 5,987,343 A 11/1999 Kinast
 5,995,858 A 11/1999 Kinast
 6,011,986 A 1/2000 Diab et al.
 6,018,673 A 1/2000 Chin et al.

6,036,642 A 3/2000 Diab et al.
 6,041,247 A 3/2000 Weckstrom et al.
 6,044,283 A 3/2000 Fein et al.
 6,081,735 A 6/2000 Diab et al.
 6,115,621 A 9/2000 Chin
 6,163,715 A 12/2000 Larsen et al.
 6,181,959 B1 1/2001 Schollermann et al.
 6,206,830 B1 3/2001 Diab et al.
 6,215,295 B1 4/2001 Smith, III
 6,226,540 B1 5/2001 Bernreuter
 6,230,035 B1 5/2001 Aoyagi et al.
 6,253,097 B1 6/2001 Aronow et al.
 6,263,222 B1 7/2001 Diab et al.
 6,272,363 B1 8/2001 Casciani et al.
 6,356,774 B1 3/2002 Bernstein et al.
 6,501,974 B1 12/2002 Huiku
 6,537,225 B1 3/2003 Mills
 6,600,940 B1 7/2003 Fein et al.
 6,611,320 B1 * 8/2003 Lindberg et al. 356/40
 6,628,975 B1 9/2003 Fein et al.
 6,667,803 B1 12/2003 Flessland et al.
 6,673,596 B1 1/2004 Sayler et al.
 2001/0005773 A1 6/2001 Larsen et al.
 2001/0020123 A1 9/2001 Diab et al.
 2001/0029326 A1 10/2001 Diab et al.
 2001/0037059 A1 11/2001 Stone et al.
 2002/0161287 A1 10/2002 Schmitt

FOREIGN PATENT DOCUMENTS

EP 0945 100 A1 9/1999
 EP 0992 214 A2 4/2000
 WO WO 02/14793 A2 2/2002

* cited by examiner

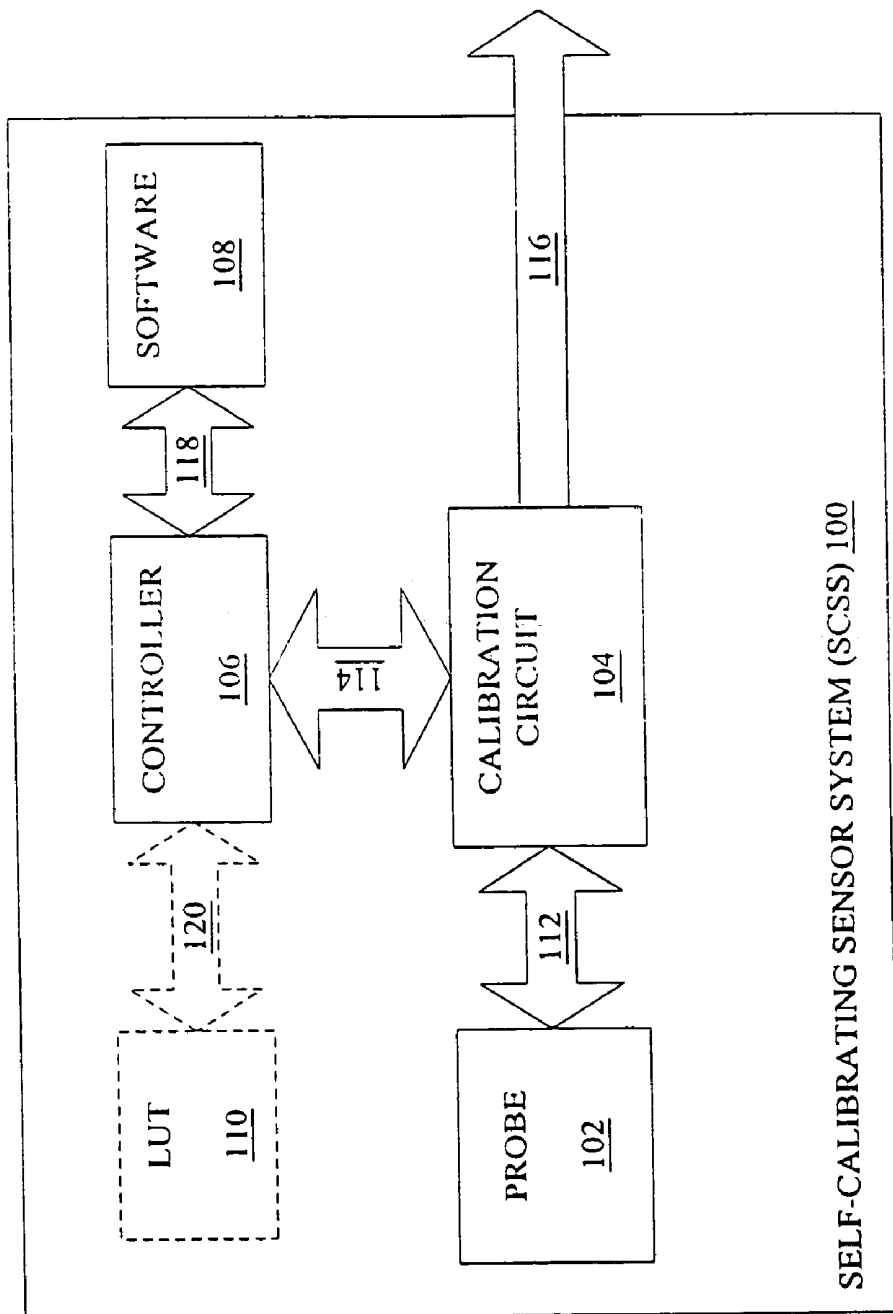


FIG. 1

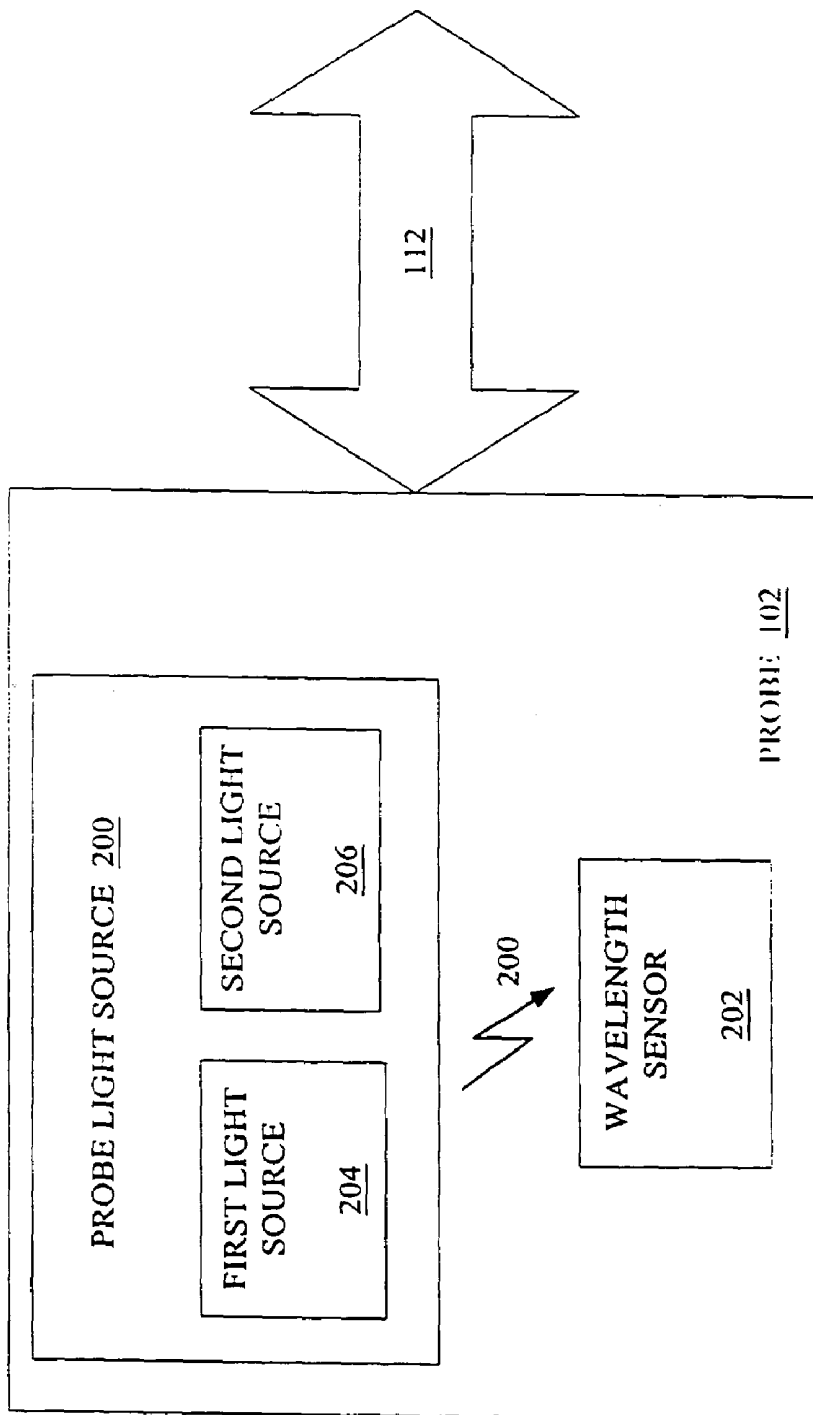


FIG. 2

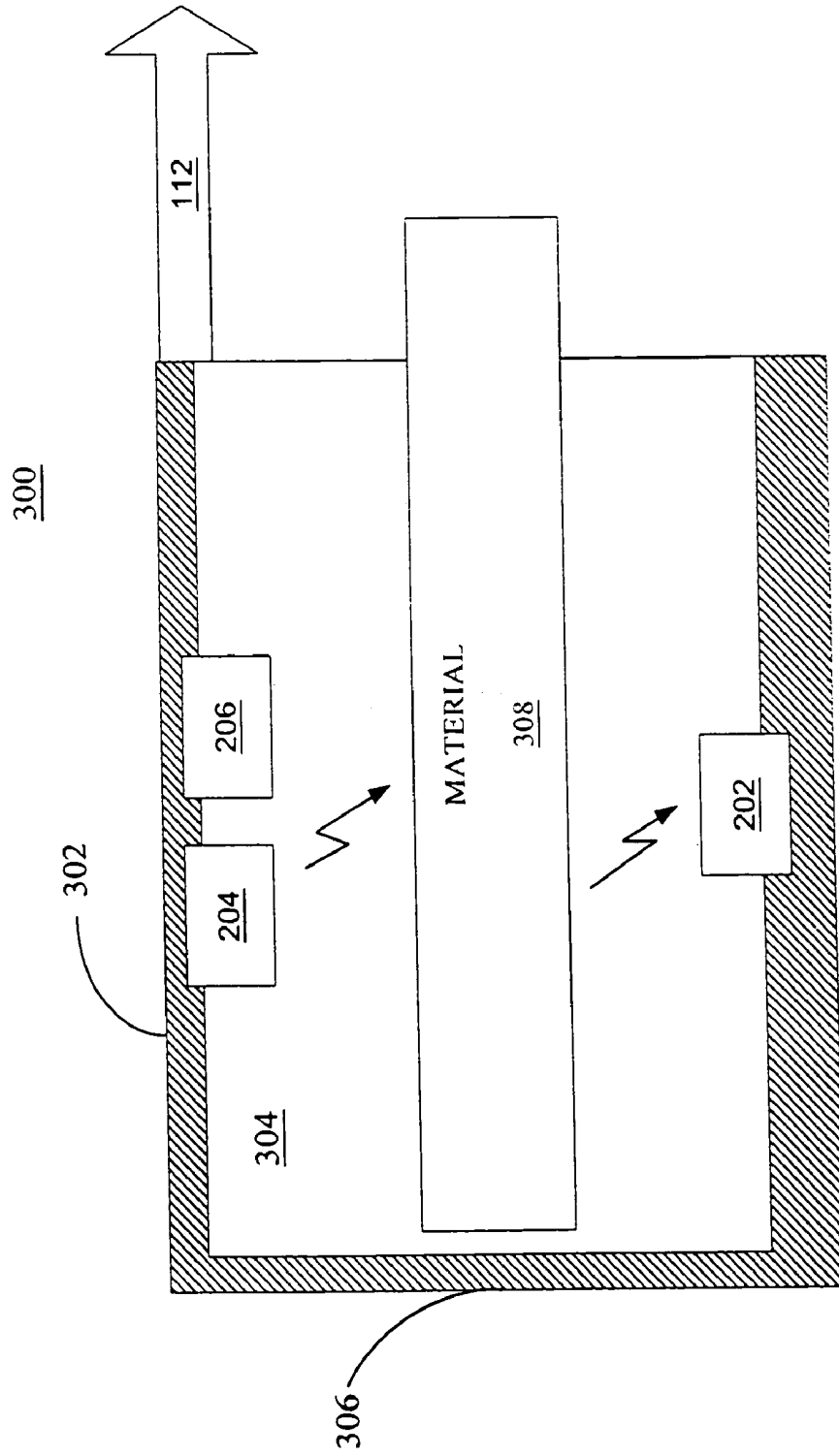


FIG. 3

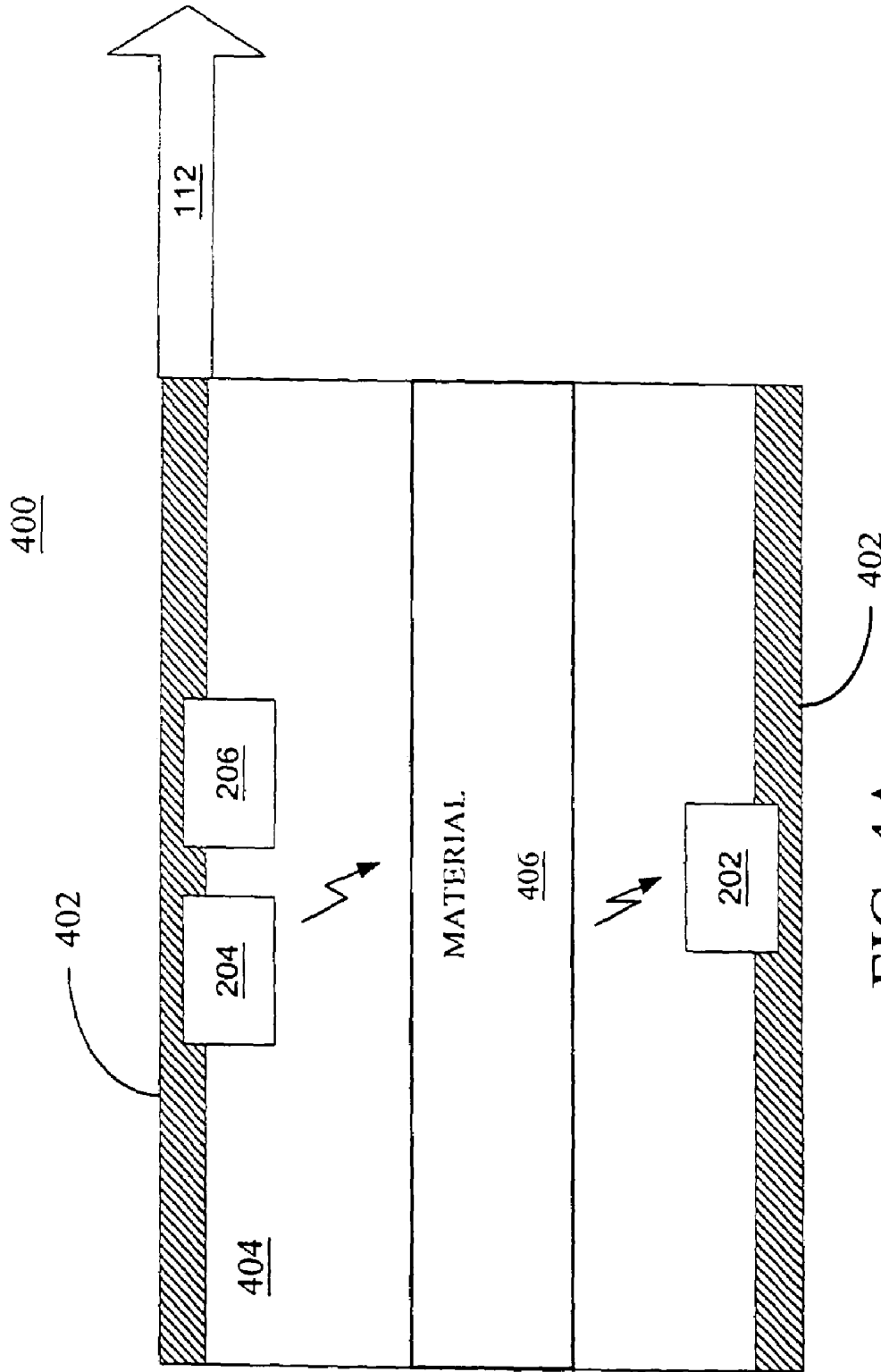


FIG. 4A

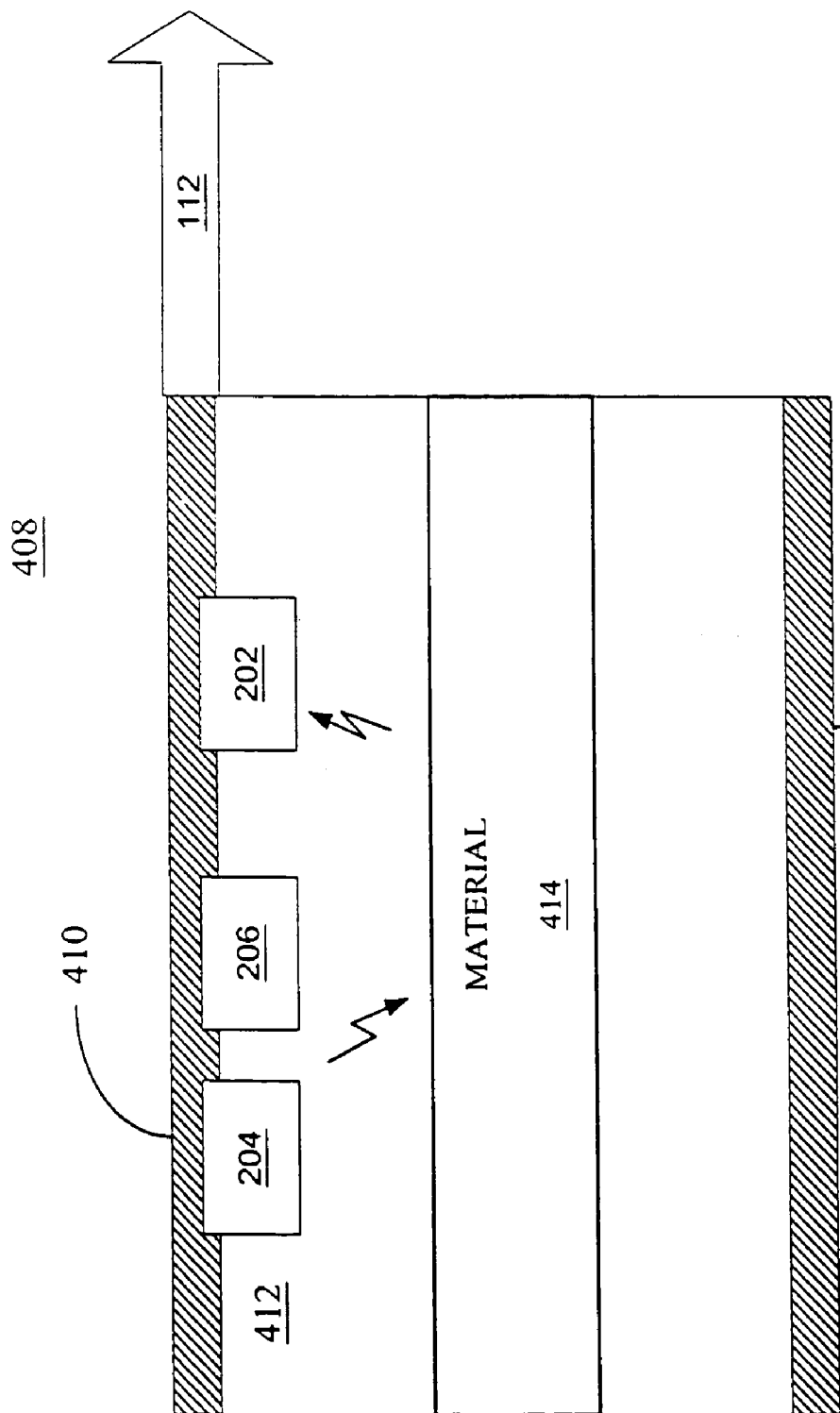


FIG. 4B

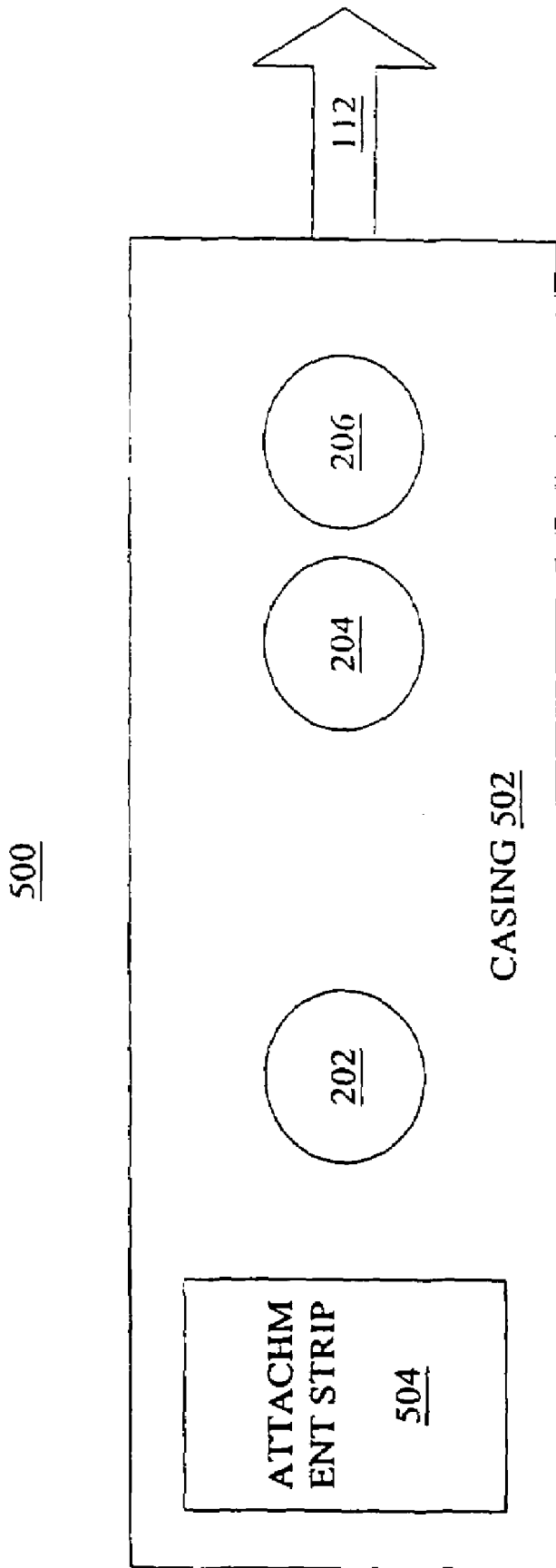


FIG. 5

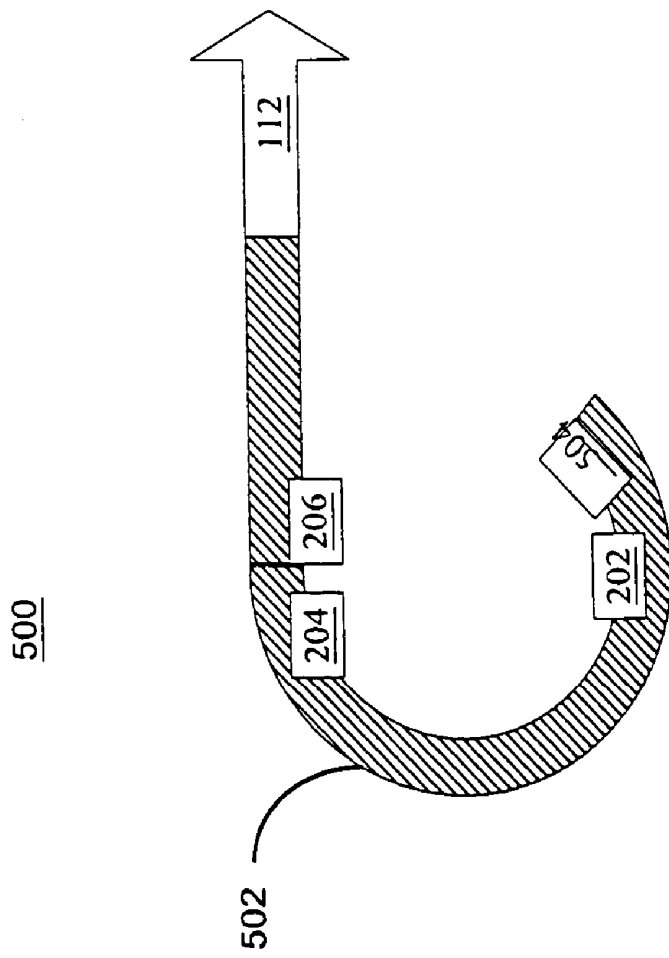


FIG. 6

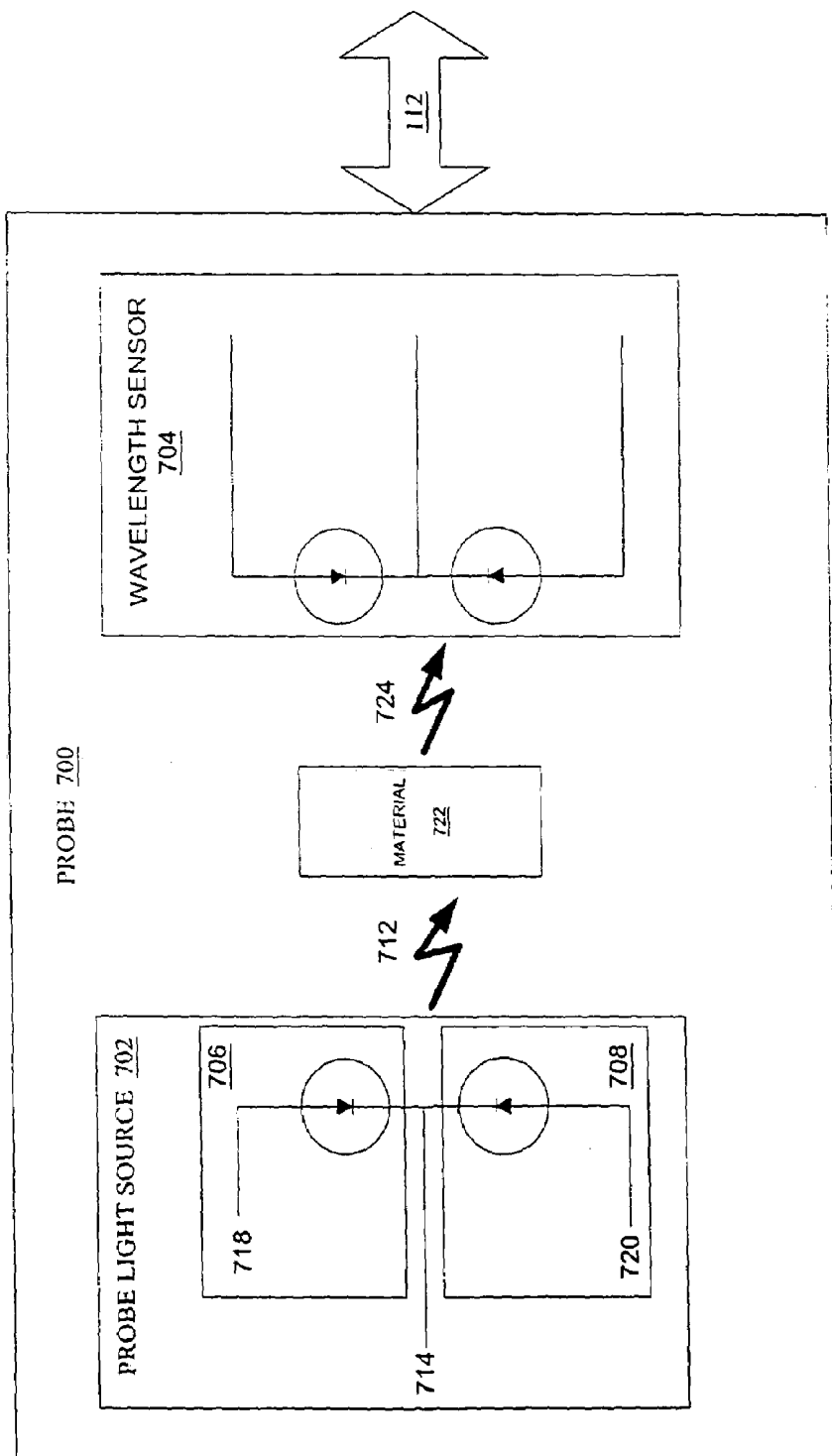


FIG. 7

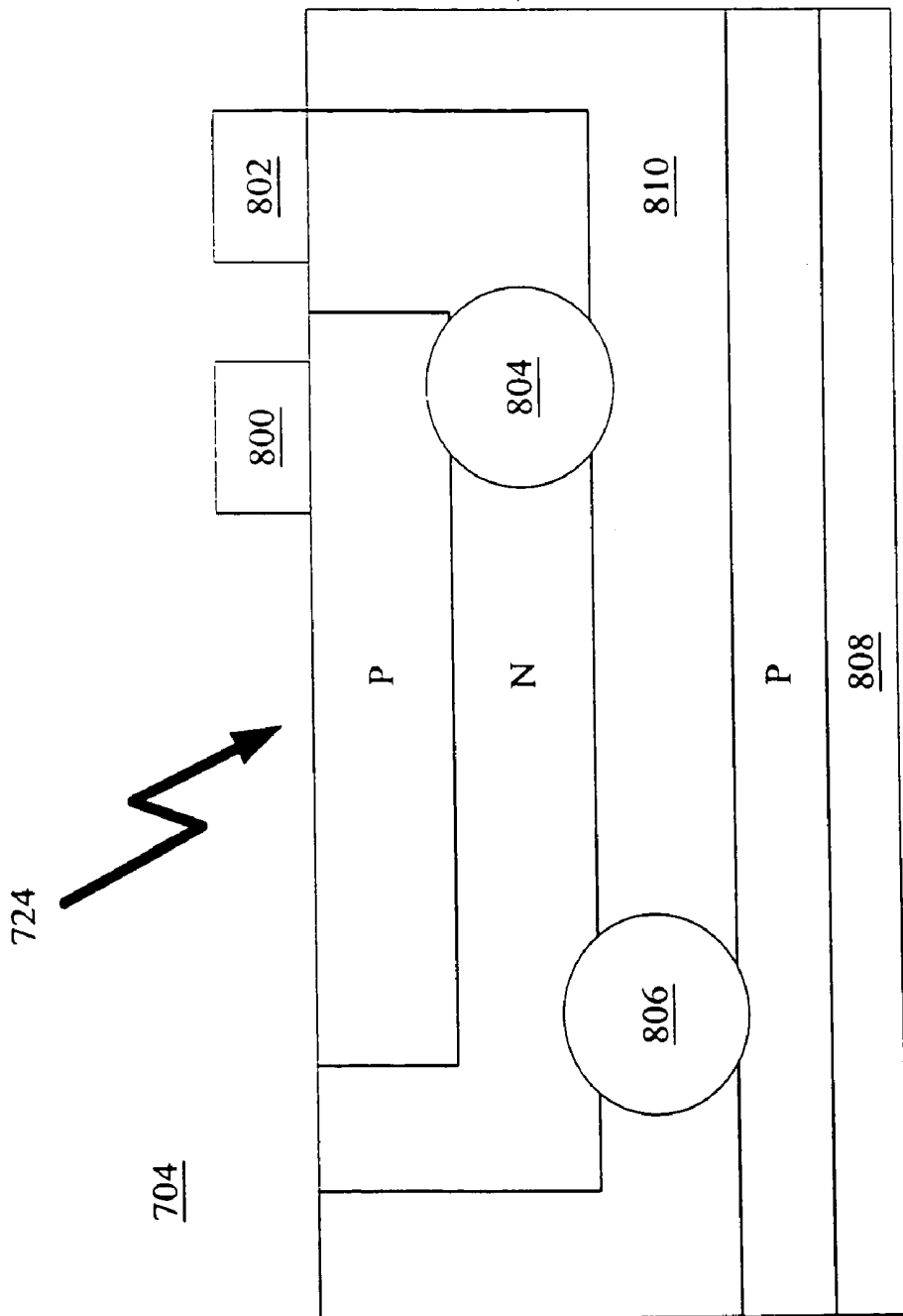


FIG. 8

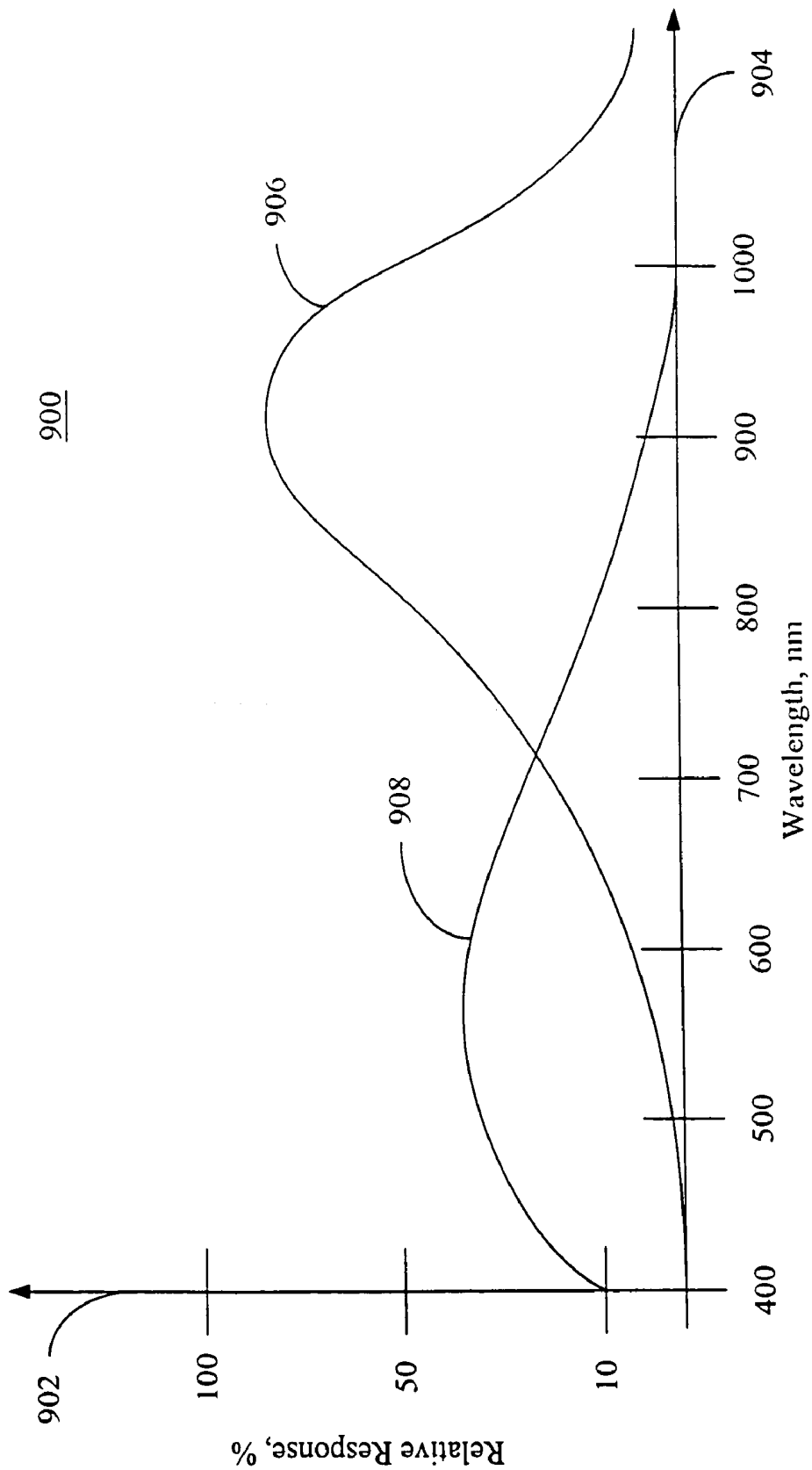


FIG. 9

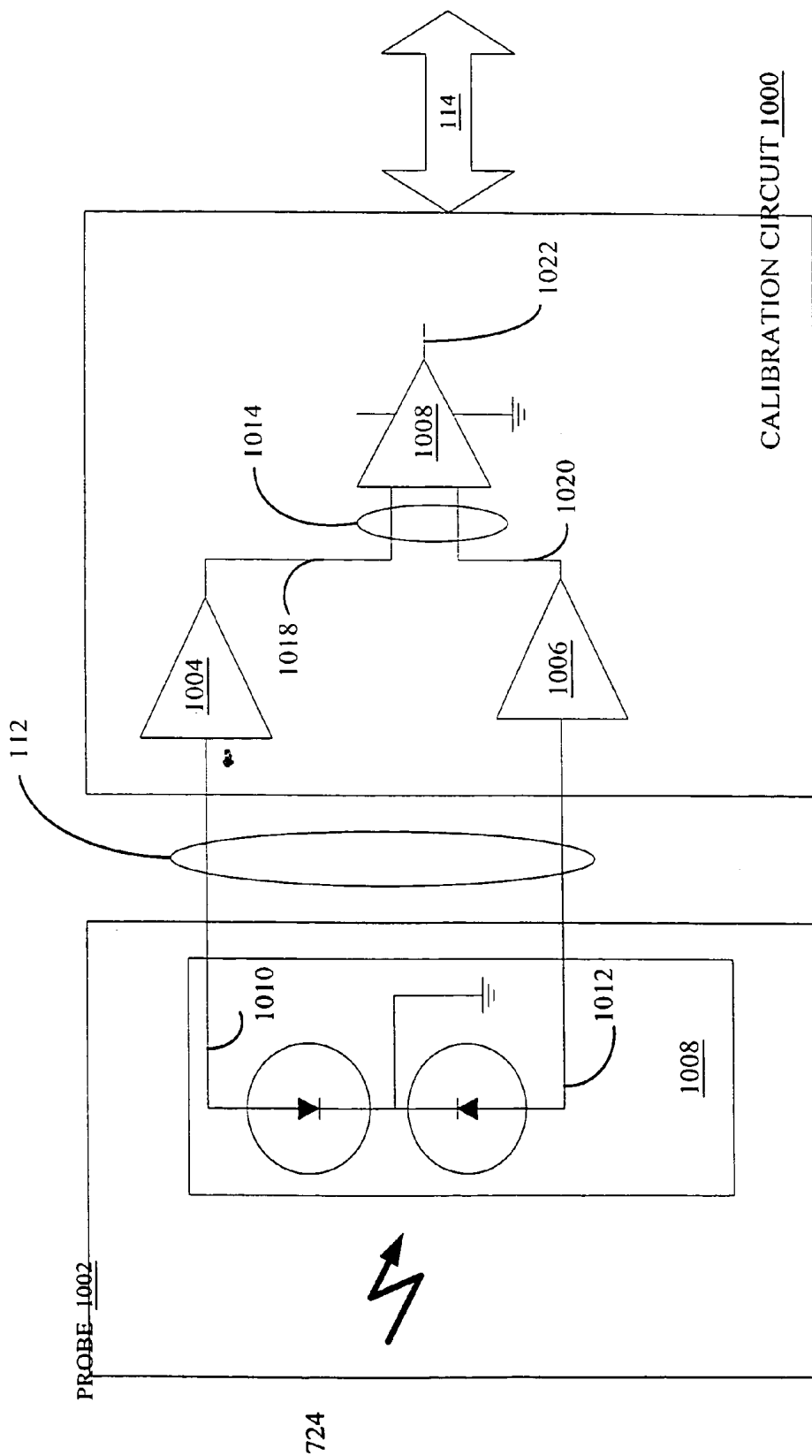


FIG. 10

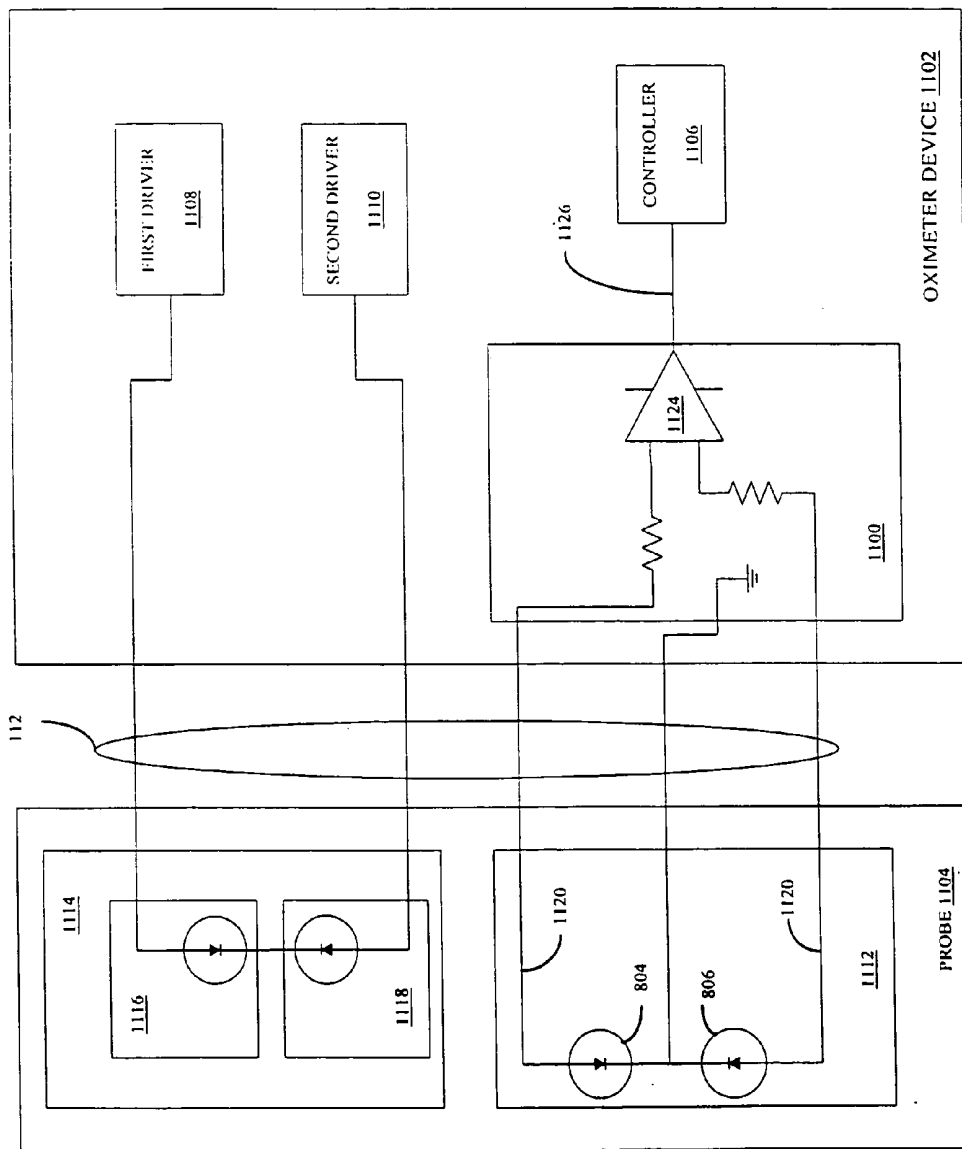


FIG. 11

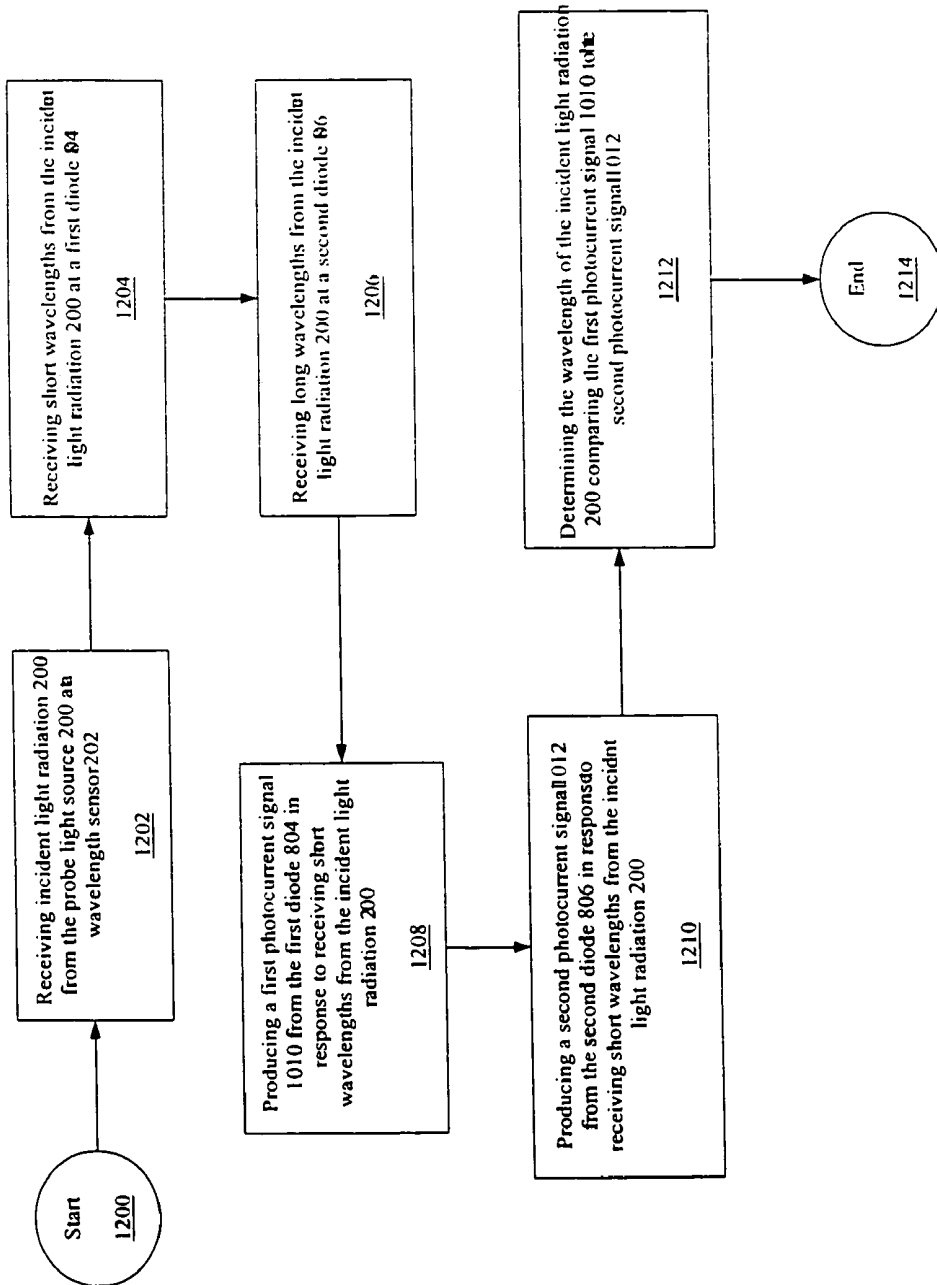


FIG. 12

SYSTEM AND METHOD FOR A SELF-CALIBRATING NON-INVASIVE SENSOR

CROSS-REFERENCE TO RELATED APPLICATIONS

This application is a continuation of U.S. patent application Ser. No. 10/149,779, filed Jun. 12, 2002 now U.S. Pat. No. 6,889,153, and entitled System and Method For A Self-Calibrating Non-Invasive Sensor, which is a continuation of International Application No., PCT/US01/25109, filed Aug. 9, 2001, and entitled System and Method For A Self-Calibrating Non-Invasive Sensor, which claims the benefit of U.S. Provisional Patent Application No. 60/225,021, filed on Aug. 11, 2001, and entitled Self Calibrating Non-Invasive Blood Component Sensor.

BACKGROUND OF THE INVENTION

1. Technical Field

This invention relates generally to non-invasive sensing devices, and in particular to calibrating these non-invasive sensing devices.

2. Related Art

Coherent light sources are utilized in a broad range of applications in many distinct fields of technology including the consumer, industrial, medical, defense and scientific fields. In the medical field an emitter-receiver pair of coherent light sources in form of light-emitting diodes (LEDs) are often utilized in medical sensing devices to obtain accurate non-invasive measurements. An example application of such a medical sensing device may include a blood constituent monitoring system and/or a non-invasive oximeter that may be utilized to monitor arterial oxygen saturation.

In non-invasive oximetry, coherent light having a known specific wavelength is typically transmitted from an emitter LED through a target, such as biological tissue carrying blood, to a photodetector. The photodetector receives and measures a portion of transmitted coherent light that is neither absorbed nor reflected from the blood in the biological tissue in order to determine the oxygen saturation (SPO₂) within the blood. Similarly, an example of an industrial application may include a non-invasive sensor system having a coherent light of a known specific wavelength transmitted from a coherent light source (such as an LED emitter) through a target, such as a fluid or material, to photodetector.

Unfortunately, these types of non-invasive sensor systems utilizing a coherent light source require accurate prior knowledge of the wavelength of the coherent light source in order to determine the amount of coherent light that is absorbed or reflected through the target. One way of having the prior knowledge of the wavelength is to select coherent light source emitters that have wavelengths within a certain range of tolerance. As such, attempts at determining the wavelength have included a binning process of selecting LEDs within the required nominal wavelength specifications.

However, it is appreciated by those skilled in the art and familiar with the production of emitter-photodiode sensing devices that there is a need to be able to select from a wider variation of emitter output wavelengths in reducing the production costs and defect rates of the sensing devices. As an example, typical production techniques require selection of an emitter within 2 nm of a target wavelength, which may lead to rejection of 40–60% of the component emitters. Moreover, an additional problem is that a selected emitter,

which was within the target wavelength at time of production, will typically degrade over time, vary with temperature, and the drive circuit may become unstable and cause a wavelength shift.

Attempts to solve the wavelength shift problem have included systems that correlate the wavelength shift to a change in drive circuit current. The change in drive circuit current drives the LED to a specific wavelength. Typically, these systems include a scheme for determining the wavelength shift of the photodiodes via a series of filters, diffusers and a plurality of photodetectors. Unfortunately, this approach is too complex and expensive for practical manufacturing techniques.

Therefore, there is a need for a non-invasive sensor system that is capable of measuring the wavelength of a light source without requiring prior knowledge of the wavelength of the light source and is not complex or expensive to manufacture.

SUMMARY

This invention is a self-calibrating sensor system “SCSS” capable of determining the actual wavelength of light emitted from a light source resulting in accurate measurements over a wide variation of wavelength ranges. In an example operation, the SCSS is capable of receiving incident light radiation from the at least one light source at a sensor probe and producing a calibrated signal corresponding to the received incident light radiation at the sensor probe.

As an example implementation of the SCSS architecture, the SCSS may include a sensor probe receiving incident light radiation from at least one light source and a calibration circuit in signal communication with the sensor probe. The calibration circuit may produce a calibrated signal corresponding to the received incident light radiation at the sensor probe. The sensor probe may include a wavelength sensor. The wavelength sensor may include a first diode configured to receive short wavelengths from the incident light radiation and produce a first photocurrent signal and a second diode configured to receive long wavelengths from the incident light radiation and produce a second photocurrent signal.

BRIEF DESCRIPTION OF THE FIGURES

The invention may be better understood with reference to the following figures. The components in the figures are not necessarily to scale, emphasis instead being placed upon clearly illustrating the principles of the invention. Moreover, in the figures, like reference numerals designate corresponding parts throughout the several views.

FIG. 1 illustrates a block diagram of an example implementation of a self-calibrating sensor system (SCSS).

FIG. 2 illustrates a block diagram of an example implementation of the probe block of the SCSS shown FIG. 1.

FIG. 3 illustrates a cross-sectional view of an example implementation of the probe shown in FIG. 2.

FIG. 4A illustrates a cross-sectional view of another example implementation of the probe shown in FIG. 2.

FIG. 4B illustrates a cross-sectional view of example reflective implementation of the probe shown in FIG. 2.

FIG. 5 is a top view of an example implementation of the probe shown in FIG. 4.

FIG. 6 is a cross-sectional view of the probe implementation of FIG. 5.

FIG. 7 illustrates an example implementation of the probe block shown in FIG. 2 utilizing photodiodes.

FIG. 8 illustrates a cross-sectional view of an example implementation of the wavelength sensor block shown in FIG. 7 utilizing a double diffusion photodiode.

FIG. 9 is a graph of the response curve of the wavelength sensor shown in FIG. 8.

FIG. 10 is schematic diagram depicting an exemplary implementation of the calibration circuit block shown in FIG. 1.

FIG. 11 is schematic diagram depicting another exemplary implementation of the calibration circuit block shown in FIG. 1.

FIG. 12 is a flow chart illustrating the process performed by the SCSS shown in FIG. 1.

DETAILED DESCRIPTION OF THE PREFERRED EMBODIMENT

FIG. 1 illustrates a block diagram of a self-calibrating sensor system (SCSS) 100. The SCSS 100 may include a probe 102, a calibration circuit 104, a controller 106, software 108 located in memory (not shown) and optional lookup table ("LUT") 110. The probe 102 is in signal communication, via signal path 112, to the calibration circuit 104. The calibration circuit 106 may be a divider and/or

comparator circuit. The calibration circuit 104 is in signal communication to the controller 106 and an external output device (not shown) via signal paths 114 and 116, respectively. The controller 106 is in signal communication to software 108 and optional LUT 110 via signal paths 118 and 120, respectively.

The controller 106 may be any general-purpose processor such as an Intel XXX86, Motorola 68XXX or PowerPC, DEC Alpha or other equivalent processor. Alternatively, a specific circuit or oriented device may selectively be utilized as the controller 106. Additionally, the controller 106 may also be integrated into a signal semiconductor chip such as an Application Specific Integrated Chip (ASIC) or Reduced Instruction Set Computer (RISC), or may be implemented via a Digital Signal Processor (DSP) chip. Examples of a specific circuit or oriented device for the controller 106 may also be a mixed sionac ASIC.

The software 108 may be resident in memory (not shown) located either internally or externally to the controller 106. The software 108 includes both logic enabling the controller 106 to operate and also logic for self-calibrating the SCSS 100.

An example of the external output device may be an oximeter such as a NPB40 manufactured by Nellcor of Pleasanton, Calif., a 9840 Series pulse oximeter manufactured by Nonin Medical, Inc. of Plymouth, Minn., or an equivalent device.

FIG. 2 shows an example implementation of probe 102. Probe 102 may include a probe light source 200 and wavelength sensor 202. Probe light source 200 may include a first light source 204 and second light source 206. First light source 204 and second light source 206 may be implemented utilizing light-emitting diodes (LEDs). As an example implementation in oximeter application, first light source 204 may be an LED emitting light radiation at a wavelength of approximately 660 nm and second light source 206 may be an LED emitting light radiation at a wavelength of approximately 880 nm. Wavelength sensor 202 may be implemented utilizing a double diffusion photodiode. It is appreciated by those of skill in the art that probe light source 200 may also include multiple light sources in the order of three or more.

In FIG. 3, a cross-sectional view of an example implementation of the probe 300 is shown. In this example, probe 300 may be a medical device such as a transmissive blood oxygen saturation and pulse rate sensor. However, it would be appreciated by one skilled in the art that probe 300 may also be a reflective sensor. Additionally, probe 300 may also be utilized for measuring other blood constituents including, but not limited to, oxyhemoglobin, bilirubin, carboxy-hemoglobin, and glucose. Probe 300 may include a rigid casing 302 having a cavity 304 and casing butt 306, first light source 204, second light source 206 and wavelength sensor 202. Probe 300 is connected to calibration circuit 104, FIG. 1, via signal path 112. A material 308, FIG. 3, such as a finger may be inserted into the cavity 304.

As an example, first light source 204 and second light source 206 may be two LED emitters that produce light radiation at a wavelength of approximately 660 nm and 880 nm, respectively. Wavelength sensor 202 is supported within the rigid casing 302 opposite first light source 204 and second light source 206. First light source 204 and second light source 206 and wavelength sensor 202 may be in signal communication with a control cable (not shown). The control cable is in signal communication with an oximeter (not shown) via signal path 112. The oximeter determines the oxygen saturation of the blood in the material 308 (in this example a finger) by measuring and processing the amount of incident light radiation reaching wavelength sensor 202 from a pulse of light radiation from first light source 204.

In operation, the SCSS 100, FIG. 1, performs a self-calibration procedure prior to measuring any of the properties of the material 308, FIG. 3. This self-calibration procedure includes emitting a pulse of light radiation from the first light source 204 that is received as incident light radiation by wavelength sensor 202 prior to inserting material 308 into the cavity 304. The oximeter utilizes the measured incident light radiation received by wavelength sensor 202 to determine the operating wavelength of the first light source 204. Once the operating wavelength of the first light source 203 is known, the SCSS 100, FIG. 1, is utilized in combination with the oximeter to accurately determine blood oxygen saturation of the material 308.

The self-calibration procedure is beneficial because it is appreciated by those skilled in the art that light radiation output by first light source 204 of 660 nm in this example implementation is in the red spectral region. It is the absorption of this red light radiation that the oximeter utilizes to determine the oxygen saturation of the blood. As such, a relatively small variation in operating wavelength may results in inaccurate readings at the oximeter. As an example, without the self-calibration procedure, if the light radiation output by first light source 204 varied in excess of ± 2 nm from an operating wavelength required by the oximeter, the results would be inaccurate.

FIG. 4A illustrates a cross-sectional view of another example implementation of probe 400. In this example, probe 400 may include a rigid or flexible casing 402 having a cavity 404, first light source 204, second light source 206 and wavelength sensor 202. Similar to the previous example implementation, probe 400 is connected to calibration circuit 104, FIG. 1, via signal path 112, however, probe 400, FIG. 4A, does not have a cavity butt. A material 406 may be inserted into the cavity 404.

Similar to the previous example, first light source 204 and second light source 206 may be two LED emitters that produce light radiation at different wavelengths. Wavelength sensor 202 is supported within the rigid casing 402 opposite first light source 204 and second light source 206. First light

source **204** and second light source **206** and wavelength sensor **202** may be in signal communication with a control cable (not shown). The control cable is in signal communication with a measuring device (not shown) via signal path **112**. The measuring device determines the properties in the material **406** by measuring and processing the amount of incident light radiation reaching wavelength sensor **202** from a pulse of light radiation from first light source **204**.

As an industrial example, the material **406** may be a fluid, liquid or solid material that exhibits optical transmissive characteristics that may be measured and utilized to determine the properties of the material. An example implementation would include measuring the properties of the material for process or quality control purposes.

Again in operation, the SCSS **100**, FIG. **1**, performs a self-calibration procedure prior to measuring any of the properties of the material **406**, FIG. **4A**. This self-calibration procedure includes emitting a pulse of light radiation from the first light source **204** that is received as incident light radiation by wavelength sensor **202** prior to inserting material **406** into the cavity **404**. The measuring device utilizes the measured incident light radiation received by wavelength sensor **202** to determine the operating wavelength of the first light source **204**. Once the operating wavelength of the first light source **204** is known, the SCSS **100**, FIG. **1**, is utilized in combination with the measuring device to accurately determine the properties of the material **406**.

FIG. **4B** illustrates a cross-sectional view of an example reflective implementation of probe **408**. In this example, probe **408** may include a rigid or flexible casing **410** having a cavity **412**, first light source **204**, second light source **206** and wavelength sensor **202**. Similar to the previous example implementation, probe **408** is connected to calibration circuit **104**, FIG. **1**, via signal path **112**, however, probe **408**, FIG. **4B**, does not have a cavity butt. A material **412** may be inserted into the cavity **412**.

Similar to the previous example, first light source **204** and second light source **206** may be two LED emitters that produce light radiation at different wavelengths. However, in this example, wavelength sensor **202** is supported within the rigid casing **410** adjacent to first light source **204** and second light source **206**. First light source **204** and second light source **206** and wavelength sensor **202** may be in signal communication with a control cable (not shown). The control cable is in signal communication with a measuring device (not shown) via signal path **112**. The measuring device determines the properties in the material **412** by measuring and processing the amount of incident light radiation reflected by material **412** and reaching wavelength sensor **202** from a pulse of light radiation from first light source **204**.

Again, as an industrial example, the material **412** may be a fluid, liquid or solid material that exhibits optical transmissive characteristics that may be measured and utilized to determine the properties of the material. An example implementation would include measuring the properties of the material for process or quality control purposes.

Again in operation, the SCSS **100**, FIG. **1**, performs a self-calibration procedure prior to measuring any of the properties of the material **412**, FIG. **4B**. This self-calibration procedure includes emitting a pulse of light radiation from the first light source **204** that is reflected by flexible casing **410** and later received as incident light radiation by wavelength sensor **202** prior to inserting material **412** into the cavity **410**. The measuring device utilizes the measured incident light radiation received by wavelength sensor **202** to determine the operating wavelength of the first light

source **204**. Once the operating wavelength of the first light source **204** is known, the SCSS **100**, FIG. **1**, is utilized in combination with the measuring device to accurately determine the properties of the material **412**.

It is appreciated by of skill in the art that it is possible to generate signals from the wavelength sensor **202**, FIG. **2** during operation of the light sources **204** and **206** through the medium (i.e., material **308**, FIG. **3**, **406**, FIG. **4A**, and/or **414**, FIG. **4B**) being inspected. It is also possible to generate the same signals using light reflected off the medium. Therefore, it is not necessary to couple the light sources **204**, FIG. **2** and **206** directly to the wavelength sensor **202** as long as the medium either transmits or reflects enough light to generate processable signals from the wavelength sensor **202**.

In FIG. **5**, a top view of an example medical implementation of probe **500** having a flexible casing (i.e., flexible strip) **502** is shown. Probe **500** may include first light source **204**, second light source **206** and wavelength sensor **202**. In this example implementation, probe **500** is a blood oxygen saturation and pulse rate sensor that utilizes the flexible strip **502** to attach to a material, such as a body part (not shown). The probe **500** is connected to an oximeter (not shown) via signal path **112**. The flexible strip **502** may be wrapped around the body part and affixed to itself via an attachment strip (such as an adhesive strip) **504**. Example body parts would include a finger, toe, ear-lobe, arm, leg or other similar parts.

As an example, first light source **204** and second light source **206** may be two LED emitters that produce light radiation at a wavelength of approximately 660 nm and 880 nm, respectively. Wavelength sensor **202** is supported within the flexible strip **502** and placed opposite first light source **204** and second light source **206** when the flexible strip **502** is wrapped around a body part. First light source **204** and second light source **206** and wavelength sensor **202** may be in signal communication with a control cable (not shown). The control cable is in signal communication with an oximeter (not shown) via signal path **112**. The oximeter determines the oxygen saturation of the blood in the body part by measuring and processing the amount of incident light radiation reaching wavelength sensor **202** from a pulse of light radiation from first light source **204**.

As before, in operation, the SCSS **100**, FIG. **1**, performs a self-calibration procedure prior to measuring any of the properties of the body part. This self-calibration procedure includes, prior to wrapping flexible strip **502** around the body part, bending the flexible strip **502** so that the first light source **204** and second light source **206** are opposite in special orientation to wavelength sensor **202** and then emitting a pulse of light radiation from the first light source **204** that is received as incident light radiation by wavelength sensor **202**. The oximeter utilizes the measured incident light radiation received by wavelength sensor **202** to determine the operating wavelength of the first light source **204**. Once the operating wavelength of the first light source **204** is known, placed around a body part and the wavelength sensor **202** measures the incident light radiation emitted by the first light source **204** and passing through the blood flowing within the body part. The SCSS **100**, FIG. **1**, is then utilized in combination with the oximeter to accurately determine blood oxygen saturation of the body part. In FIG. **6**, a cross-sectional view of the probe **500** is shown in a wrap type position.

In FIG. **7**, an example implementation of the probe **700** is shown utilizing photodiodes. Similar to FIG. **2**, Probe **700**, FIG. **7**, includes probe light source **702** and wavelength

sensor **704**. Probe light source **702** includes first light source **706** and second light source **708**. First light source **706** may include LED **710** and second light source may include LED **712**. Wavelength sensor **704** is a double diffusion photodiode.

As an example of operation, LED **710** and LED **712** may have their cathodes grounded in common at signal path **714** and may emit light radiation **716** at wavelengths 660 nm and 880 nm, respectively, when a voltage is applied at anodes **718** and **720**, respectively. The emitted light radiation **716** is incident on material **722**. A part of the emitted light radiation **716** is transmitted through material **722** and is received as incident light radiation **724** by wavelength sensor **704**. As before, in order to properly measure the properties of the material **722** from the received incident light radiation **724**, the SCSS **100**, FIG. **1** performs a self-calibration procedure.

The SCSS **100**, FIG. **1**, performs a self-calibration procedure prior to measuring any of the properties of the material **722**. This self-calibration procedure includes emitting a pulse of light radiation **716** from LED **710** that is received as incident light radiation **724** by wavelength sensor **704** prior to inserting material **722** between the probe light source **702** and wavelength sensor **704**. The oximeter utilizes the measured incident light radiation **724** received by wavelength sensor **704** to determine the operating wavelength of LED **710**. Once the operating wavelength of LED **710** is known, the SCSS **100**, FIG. **1**, is utilized in combination with the oximeter to accurately determine blood oxygen saturation of the material **722**.

FIG. **8** illustrates a cross-sectional view of the wavelength sensor **704** receiving incident light radiation **724** utilizing a double diffusion photodiode (also known as a double junction photodiode). Photodiodes with double diffusion are typically utilized to accurately measure the centroid wavelength of light sources such as LEDs **710** and **712**. Double diffusion photodiodes are processed with two junctions, one on the top surface and one on the back surface of a semiconductor photodiode (such as a Si-photodiode), each junction typically exhibits a different and well-defined spectral response. As result, by measuring the quotient of signals generated by the two junctions, the centroid wavelength of any given monochromatic light source may be determined.

The wavelength sensor **704** has two p-n junctions constructed vertically on a common silicon substrate. The wavelength sensor **704** includes a first anode **800**, common cathode **802**, first diode **804** (also known as an upper diode), second diode **806** (also known as a lower diode), second anode **808**, and a thin active region **810**. The first anode **800** is positioned on the top surface above the common cathode **802** forming the first diode **804**. The thickness of the first diode **804** is chosen so that the energy of the shortest wavelength being measured from the incident light radiation **724** is absorbed entirely therein. The second diode **806** is formed between the common cathode **802** and the second anode **808** that placed on the bottom surface with the thin active region **810** between the common cathode **802** and the second anode **808**. The thickness of the thin active region **810** is selected to allow for absorption of substantially all of the longest measured wavelength of incident light radiation **724**.

FIG. **9** illustrates a typical plot **900** of the spectral response of the wavelength sensor **704**, FIG. **8**. The plot **900**, FIG. **9**, has a vertical axes **902** representing relative response, in percentage, of the wavelength sensor **704**, FIG. **8**, and a horizontal axis **904**, FIG. **9**, representing the wavelength of the incident light radiation **724**, FIG. **8**. The plot **900**, FIG. **9**, shows two response curves **906** and **908**

representing the relative response versus wavelength for the first diode **804**, FIG. **8**, and the second diode **806**, respectively.

As an example of operation of the wavelength sensor **704**, the first diode **804** may have an enhanced blue response and the second diode **806** may have an enhanced red response. In this example, the absorbed radiation of the incident light radiation **724** between the red and blue responses (such as between 450 and 900 nm) generates two photocurrent signals proportional to the wavelength of the incident light radiation **724**. The quotient of these photocurrent signals is independent of the light level up to the saturation point of the wavelength sensor **704**. Utilizing this example, the wavelength of either monochromatic incident light radiation **724** or the spectral density peak of polychromatic incident light radiation **724** may be determined. An example of the wavelength sensor **704** may be a PSS WS-7.56 wavelength sensor produced by Pacific Silicon Sensor, Inc. of Westlake Village, Calif.

In FIG. **10**, a schematic diagram depicting an exemplary implementation of the calibration circuit **1000** is shown. The calibration circuit **1000** is in signal communication with the probe **1002** and controller **106**, FIG. **1**, via signal paths **112** and **114**, respectively. The calibration circuit **1000** may include a pair of amplifiers **1004** and **1006** (such as log amplifiers) in signal communication with first anode **800**, FIG. **8** and second anode **808** of wavelength sensor **1008**, FIG. **10**, and a differential amplifier **1010**, via signal paths **1010**, **1012** and **1014**, respectively. The differential amplifier **1008** is in signal communication with the controller **106**, FIG. **1**, via signal path **112**.

In operation, the wavelength sensor **1004** produces two photocurrent signals from the two junctions (i.e., photodiodes **804** and **806**) in the double diffusion photodiode. Each junction in the wavelength sensor **1004** exhibits a different and well-defined spectral response, which is known to the controller **106**, FIG. **1**, and the magnitude of these two resulting photocurrent signals are proportional to the wavelength of the measured incident light radiation **724**, which corresponds to one of the light sources (either **204** or **206**, FIG. **2**) in probe **1002**, FIG. **10**. The photocurrent signals are amplified by amplifiers **1004** and **1006** via signal paths **1010** and **1012**, respectively, and input into the differential amplifier **1008** via signal path **1018** and **1020**. If the amplified photocurrent signals **1018** and **1020** are approximately equal the corresponding differential output signal **1022** of the differential amplifier **1008** is almost equal to zero. Once the differential output signal **1022** is almost equal to zero the wavelength of the incident light radiation is determined and the SCSS **100**, FIG. **1**, is calibrated.

When the amplified photocurrent signals **1018** and **1020** are not approximately equal the corresponding differential output signal **1022** will vary according to the difference in magnitude value between the amplified photocurrent signals **1018** and **1020**. The differential output signal **1022** is the utilized as a reference by the controller **106**, FIG. **1**. The controller **106** determines the wavelength of the incident light radiation **724** by knowing the spectral response of the photodiodes **804** and **806**, FIG. **8**. The controller **106** either determines the wavelength of the incident light radiation **724** utilizing software **108** or other hardware (not shown) located in the SCSS **100**. The software **108** may include logic that allows the controller **106** to calculate the wavelength values in real-time from the measure values received from the wavelength sensor **1004**.

Alternatively, the controller **106** may determine the wavelength of the incident light radiation **724** utilizing the lookup

(“LUT”) table **110**. The LUT **110** may be resident in memory (not shown) resident either internally or externally to the controller **106**. The LUT **110** includes a tabulation of known spectral response in voltage versus wavelength for each photodiode **804** and **806**, FIG. **8**. Once the controller **106** measures the differential output signal **1022**, FIG. **10**, the software **108**, FIG. **1**, compares the value of the differential output signal **1022**, FIG. **10**, against values stored in the LUT **110**, FIG. **1**, and then retrieves a corresponding wavelength value. The controller **106** then utilizes the retrieved wavelength wave to self-calibrate the SCSS **100**.

Besides self-calibration, the SCSS **100** is also capable of temperature compensating for variation in the wavelength of the incident light radiation **724** due to temperature variations. The SCSS **100** may compensate for temperature variations by the same process utilized to self-calibrate.

FIG. **11** is another exemplary implementation of the SCSS **100**, FIG. **1**, with the calibration circuit **1100**, FIG. **11**, in an oximeter device **1102**. The oximeter device **1102** is in signal communication with probe **1104**, via signal path **112**, and includes calibration circuit **1100**, controller **1106**, first driver **1108** and second driver **1110**. The probe **1104** includes wavelength sensor **1112** and probe light source **1114** having first light source **1116** and second light source **1118**.

In operation, the first driver **1108** drives the first light source **1116** and the second driver **1110** drives the second light source **1118**. First light source **1116** and the second light source **1118** may individually produce light radiation which is incident of the wavelength sensor **1112**. The wavelength sensor **1112** produces two photocurrent signals from the two junctions (i.e., photodiodes **804** and **806**) in the double diffusion photodiode. Again, each junction in the wavelength sensor **1112** exhibits a different and well-defined spectral response, which is known to the controller **1106** and the magnitude of these two resulting photocurrent signals are proportional to the wavelength of the measured incident light radiation, which corresponds to one of the light sources (either **1116** or **1118**) in probe **1104**. The photocurrent signals **1120** and **1122** processed and input into the differential amplifier **1224**. If the photocurrent signals **1120** and **1122** are approximately equal the corresponding differential output signal **1126** of the differential amplifier **1224** is almost equal to zero. Once the differential output signal **1126** is almost equal to zero the wavelength of the incident light radiation is determined and the SCSS **100**, FIG. **1**, is calibrated.

When the photocurrent signals **1120** and **1122** are not approximately equal the corresponding differential output signal **1126** will vary according to the difference in magnitude value between the photocurrent signals **1120** and **1122**. The differential output signal **1126** is utilized as a reference by the controller **1106**. The controller **1106** determines the wavelength of the incident light radiation by knowing the spectral response of the photodiodes **804** and **806**. The controller **1106** either determines the wavelength of the incident light radiation utilizing software **108**, FIG. **1**, or other hardware (not shown) located in the SCSS **100**. The software **108** may include logic that allows the controller **1106**, FIG. **11**, to calculate the wavelength values in real-time from the measure values received from the wavelength sensor **1112**.

Alternatively, the controller **1106** may determine the wavelength of the incident light radiation utilizing the lookup LUT **110**, FIG. **1**. The LUT **110** may be resident in memory (not shown) resident either internally or externally to the controller **1106**, FIG. **11**. The LUT **110**, FIG. **1**, includes the tabulation of known spectral response in volt-

age versus wavelength for each photodiode **804** and **806**. Once the controller **1106** measures the differential output signal **1126**, FIG. **11**, the software **108**, FIG. **1**, compares the value of the differential output signal **1126**, FIG. **11**, against values stored in the LUT **110**, FIG. **1**, and then retrieves a corresponding wavelength value. The controller **1106**, FIG. **11**, then utilizes the retrieved wavelength wave to self-calibrate the SCSS **100**, FIG. **1**.

FIG. **12** illustrates the process performed by the SCSS **100**, FIG. **1**. The process begins in step **1200**, FIG. **12**. In step **1202**, the wavelength sensor **202**, FIG. **2**, receives incident light radiation **200** from the probe light source **200**. Within the wavelength sensor **202**, the first diode **804**, FIG. **8**, receives short wavelengths from the incident light radiation **200**, in step **1204**, FIG. **12**, and the second diode **806**, FIG. **8**, receives long wavelengths from the incident light radiation **200** in step **1206**, FIG. **12**. In step **1208**, the first diode **804** produces a first photocurrent signal **1010**, FIG. **10**, in response to receiving short wavelengths from the incident light radiation **200** and the second diode **806** produces a second photocurrent signal **1012**, FIG. **10**, in response to receiving short wavelengths from the incident light radiation **200** in step **1210**, FIG. **12**. Finally, in step **1212**, the calibration circuit **104** and/or controller **106**, FIG. **1**, determine the wavelength of the incident light radiation **200** by comparing the first photocurrent signal **1010** to the second photocurrent signal **1012**. The process then ends in step **1214**.

The SCSS **100** may be selectively implemented in software, hardware, or a combination of hardware and software. For example, the elements of the SCSS **100** may be implemented in software **108** stored in a memory (not shown) located in a controller **106**. The controller **106** may be in signal communication with a DSP or ASIC chip via communication link **112** (which may selectively be a system bus). The software **108** configures and drives the DSP or ASIC chip and performs the steps illustrated in FIG. **12**.

The software **108** comprises an ordered listing of executable instructions for implementing logical functions. The software **108** may be embodied in any computer-readable medium for use by or in connection with an instruction execution system, apparatus, or device, such as a computer-executed system, processor-containing system, or other system that may selectively fetch the instructions from the instruction execution system, apparatus, or device and execute the instructions. In the context of this document, a “computer-readable medium” is any means that may contain, store, communicate, propagate, or transport the program for use by or in connection with the instruction execution system, apparatus, or device. The computer readable medium may be for example, but not limited to, an electronic, magnetic, optical, electromagnetic, infrared, or semiconductor system, apparatus, device, or propagation medium. More specific examples (a non-exhaustive list) of the computer-readable medium would include the following: an electrical connection (electronic) having one or more wires, a portable computer diskette (magnetic), a RAM (electronic), a read-only memory (ROM) (electronic), an erasable programmable read-only memory (EPROM or Flash memory) (electronic), an optical fiber (optical), and a portable compact disc read-only memory (CDROM) (optical). Note that the computer-readable medium may even be paper or another suitable medium upon which the program is printed, as the program can be electronically captured, via for instance optical scanning of the paper or other medium, then compiled, interpreted or otherwise processed in a suitable manner if necessary, and then stored in a computer memory.

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While various implementations of the application have been described, it will be apparent to those of ordinary skill in the art that many more embodiments and implementations are possible that are within the scope of the invention. Accordingly, the invention is not to be restricted except in light of the attached claims and their equivalents.

What is claimed is:

1. A sensor system comprising:
 - a probe comprising a light source and a sensor, the sensor having a probe calibration output and a calibrated probe output, wherein the probe outputs are responsive to incident light radiation received from the light source to produce signals proportional to an amplitude and a centroid wavelength of the incident light, and the probe calibration output is generated continuously while taking a physiological measurement;
 - a calibration circuit in signal communication with the probe and comprising an electronic calibration output responsive to the probe calibration output, and a calibrated electronic output responsive to the calibrated probe output;
 - a controller in signal communication with the calibration circuit and comprising a lookup table having a wavelength value output responsive to the electronic calibration output and the calibrated electronic output, wherein the wavelength value output is determined in real-time and is then used to correct physiological data derived from the signal proportional to the amplitude of the incident light; and,
 - a measuring device comprising an output generated in response to the wavelength value output.
2. The sensor system of claim 1, wherein the physiological measurement and the output of the measuring device is oxygen saturation within blood.
3. The sensor system of claim 1, further comprising software that operates on the controller.
4. The sensor system of claim 3, the software comprising instructions for compensating for wavelength variation of the incident light radiation caused by changes in temperature.
5. The sensor system of claim 1, wherein the incident light radiation is coherent.
6. A sensor system comprising:
 - a probe comprising a light source and a sensor, the sensor having a probe calibration output and a calibrated probe output, wherein the probe outputs are responsive to incident light radiation received from the light source to produce signals proportional to an amplitude and a centroid wavelength of the incident light, and the probe calibration output is generated continuously while taking a physiological measurement;
 - a calibration circuit in signal communication with the probe and comprising an electronic calibration output responsive to the probe calibration output, and a calibrated electronic output responsive to the calibrated probe output;
 - a controller in signal communication with the calibration circuit and comprising a software-based logic responsive to the electronic calibration output and the calibrated electronic output to produce a wavelength value output is then used to correct physiological data derived from the signal proportional to the amplitude of the incident light; and,
 - a measuring device comprising an output generated in response to the wavelength value output.

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7. The sensor system of claim 6, wherein the physiological measurement and the output of the measuring device are oxygen saturation within blood, cardiac output, blood pressure, or vital signs.

8. The sensor system of claim 6, further comprising software that operates on the controller.

9. The sensor system of claim 8, the software comprising instructions for compensating for wavelength variation of the incident light radiation caused by changes in temperature.

10. The sensor system of claim 6, wherein the incident light radiation is coherent.

11. A sensor system comprising:

- a probe comprising a light source and a sensor, the sensor having a probe calibration output and a calibrated probe output, wherein the probe outputs are responsive to incident light radiation received from the light source to produce signals proportional to an amplitude and a centroid wavelength of the incident light, and the probe calibration output is generated continuously while taking a physiological measurement;
 - a calibration circuit in signal communication with the probe and comprising an electronic calibration output responsive to the probe calibration output, and a calibrated electronic output responsive to the calibrated probe output;
 - a controller in signal communication with the calibration circuit and comprising logic responsive to the electronic calibration output to provide an output to adjust light source temperature and to produce a wavelength value output that is determined in real-time and is then used to correct physiological data derived from the signal proportional to the amplitude of the incident light; and,
 - a measuring device comprising an output generated in response to the wavelength value output.
12. The sensor system of claim 11, wherein the physiological measurement and the output of the measuring device are oxygen saturation within blood, cardiac output, blood pressure, or vital signs.

13. The sensor system of claim 11, further comprising software that operates on the controller.

14. The sensor system of claim 13, the software comprising instructions for compensating for wavelength variation of the incident light radiation caused by changes in temperature.

15. The sensor system of claim 11, wherein the incident light radiation is coherent.

16. A sensor system comprising:

- a probe comprising a light source and a sensor, the sensor having a probe calibration output and a calibrated probe output, wherein the probe outputs are responsive to incident light radiation received from the light source to produce signals proportional to an amplitude and a centroid wavelength of the incident light, and the probe calibration output is generated prior to taking a physiological measurement;
- a calibration circuit in signal communication with the probe and comprising an electronic calibration output responsive to the probe calibration output, and a calibrated electronic output responsive to the calibrated probe output;
- a controller in signal communication with the calibration circuit and comprising logic responsive to the electronic calibration output and the calibrated electronic output to produce a wavelength value output that is used to determine, in real-time, the physiological mea-

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surement, and is then used to correct physiological data derived from the signal proportional to the amplitude of the incident light.

17. The sensor system of claim 16, wherein the physiological measurement is oxygen saturation within blood, cardiac output, blood pressure, or vital signs.

18. The sensor system of claim 16, further comprising software that operates on the controller.

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19. The sensor system of claim 18, the software comprising instructions for compensating for wavelength variation of the incident light radiation caused by changes in temperature.

20. The sensor system of claim 16, wherein the incident light radiation is coherent.

* * * * *

UNITED STATES PATENT AND TRADEMARK OFFICE
CERTIFICATE OF CORRECTION

PATENT NO. : 7,124,048 B2
APPLICATION NO. : 11/007656
DATED : October 17, 2006
INVENTOR(S) : Dietiker


Page 1 of 1

It is certified that error appears in the above-identified patent and that said Letters Patent is hereby corrected as shown below:

On the Title page of the patent, line 60, item 60, the line should read --Provisonal application No. 60/225,021, filed on August 11, 2000-- and not August 11, 2001.

Signed and Sealed this

Ninth Day of January, 2007

A handwritten signature in black ink on a light gray dotted background. The signature reads "Jon W. Dudas" in a cursive style.

JON W. DUDAS

Director of the United States Patent and Trademark Office

专利名称(译)	用于自校准非侵入式传感器的系统和方法		
公开(公告)号	US7124048	公开(公告)日	2006-10-17
申请号	US11/007656	申请日	2004-12-08
[标]申请(专利权)人(译)	DIETIKER THOMAS		
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[标]发明人	DIETIKER THOMAS		
发明人	DIETIKER, THOMAS		
IPC分类号	G01D18/00 A61B5/00 G01N21/27		
CPC分类号	A61B5/14546 A61B5/14551 A61B5/14552 A61B5/1495 G01J9/00 G01N21/274 G01N21/35 A61B5/14532 G01J1/08 G01J2003/2866 G01N2021/3144 G01N2201/1211 G01N2201/12723 H01L27/14647 H01L31/03529 G01N21/3504 G01N21/3563 G01N21/3577		
审查员(译)	BARLOW, 约翰		
优先权	60/225021 2000-08-11 US		
其他公开文献	US20060122801A1		
外部链接	Espacenet USPTO		

摘要(译)

一种非侵入式发射极 - 光电二极管传感器，其能够提供与所发射的光的实际波长相对应的数据流，从而允许校准传感器信号处理设备并且导致在发射器波长范围的更宽变化上的精确测量。

