

US006767327B1

(12) **United States Patent**
Corl et al.

(10) **Patent No.:** **US 6,767,327 B1**
(45) **Date of Patent:** ***Jul. 27, 2004**

(54) **METHOD OF MEASURING BLOOD PRESSURE AND VELOCITY PROXIMALLY AND DISTALLY OF A STENOSIS**

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(*) Notice: Subject to any disclaimer, the term of this patent is extended or adjusted under 35 U.S.C. 154(b) by 0 days.

This patent is subject to a terminal disclaimer.

(21) Appl. No.: **09/644,111**

(22) Filed: **Aug. 21, 2000**

Related U.S. Application Data

(63) Continuation of application No. 08/912,879, filed on Aug. 15, 1997, now Pat. No. 6,106,476, which is a continuation-in-part of application No. 08/710,062, filed on Sep. 9, 1996, now Pat. No. 5,715,827, which is a continuation of application No. 08/300,445, filed on Sep. 2, 1994, now abandoned.

(51) **Int. Cl.⁷** **A61B 5/00**
(52) **U.S. Cl.** **600/486**
(58) **Field of Search** 600/486, 488, 600/505

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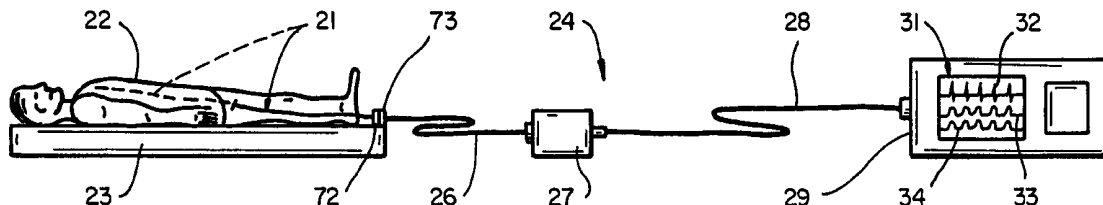
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(57) **ABSTRACT**

A method of measuring blood pressure and velocity proximally and distally of a stenosis in a vessel carrying blood includes the steps of providing a guide wire having both a pressure sensor and a velocity sensor disposed on a distal region of the guide wire, introducing the guide wire into the vessel, advancing the guide wire to position the pressure sensor and the velocity sensor proximally and distally of the stenosis, and measuring the blood pressure and velocity proximally and distally of the stenosis with the pressure sensor and the velocity sensor.

28 Claims, 6 Drawing Sheets



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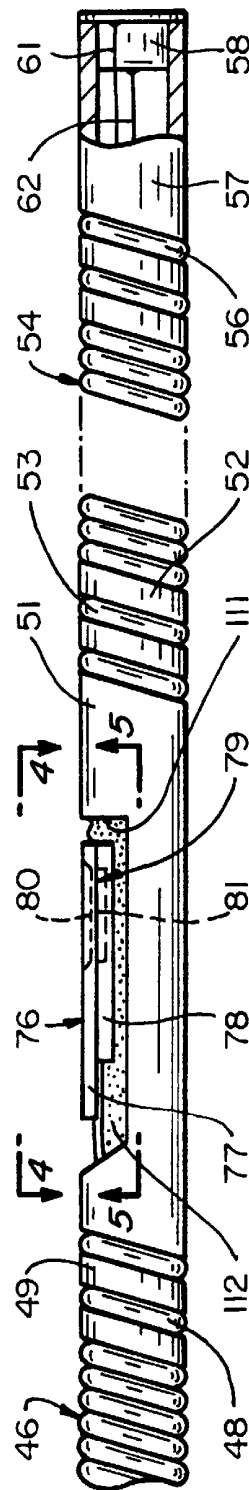
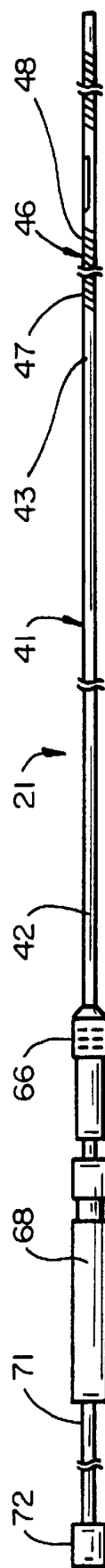
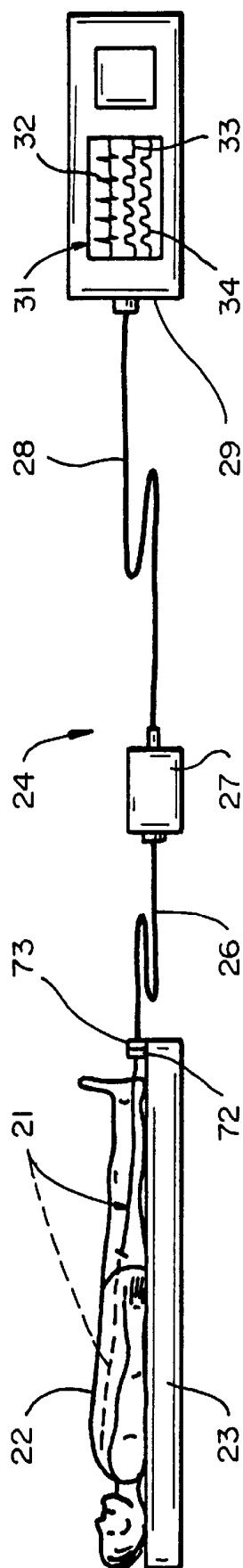
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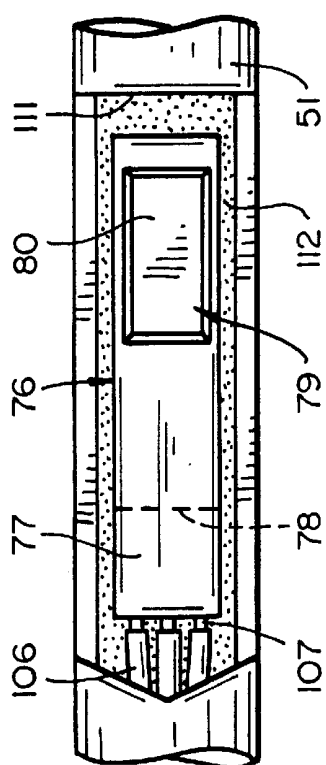


FIG-4

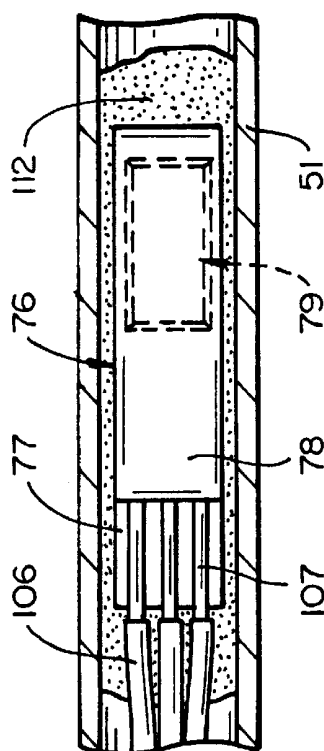


FIG-5

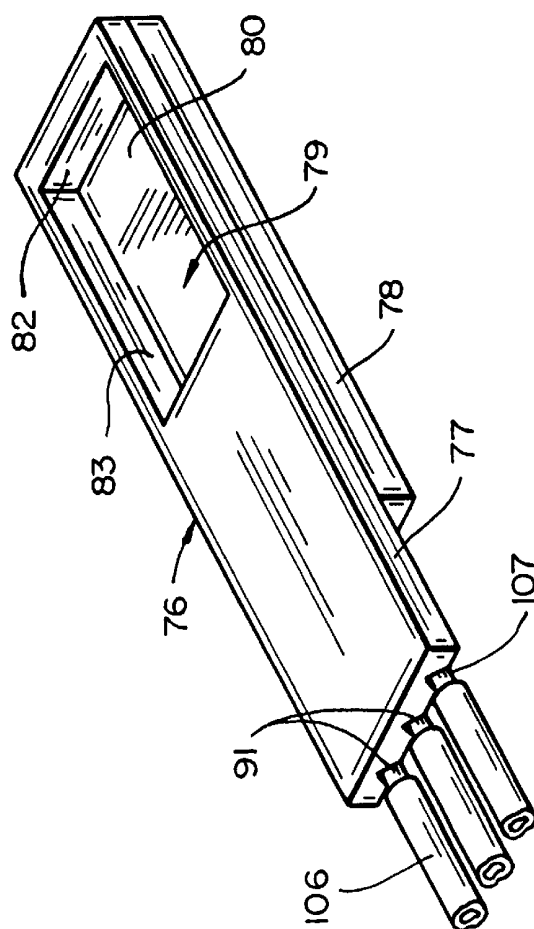


FIG-6

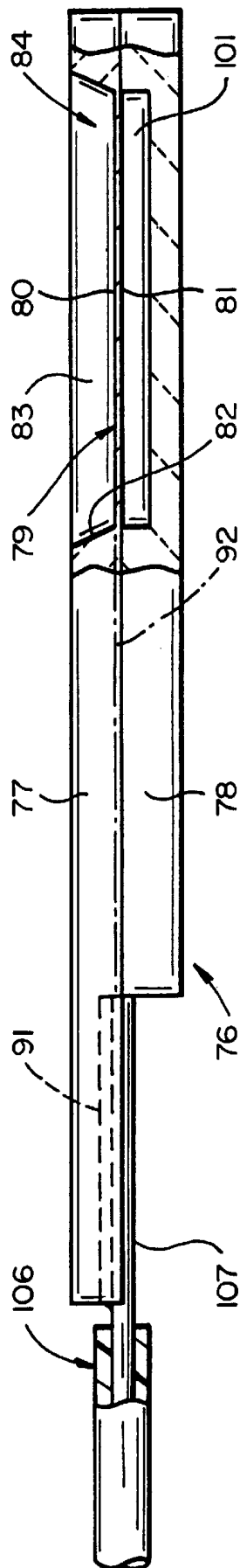
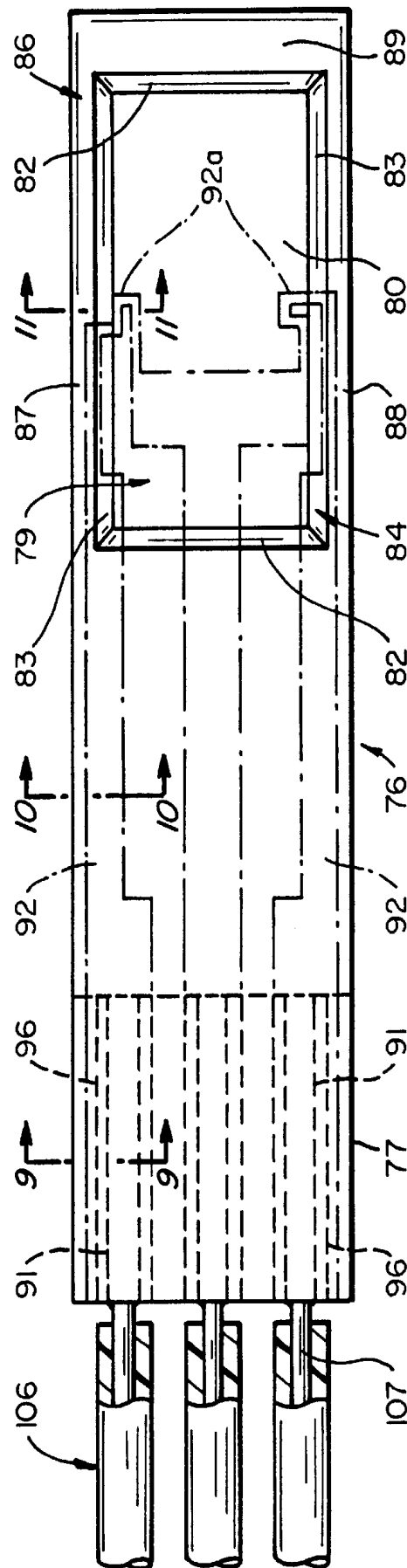
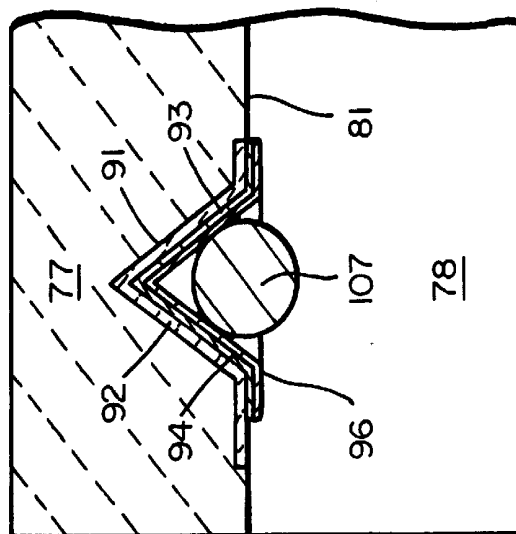


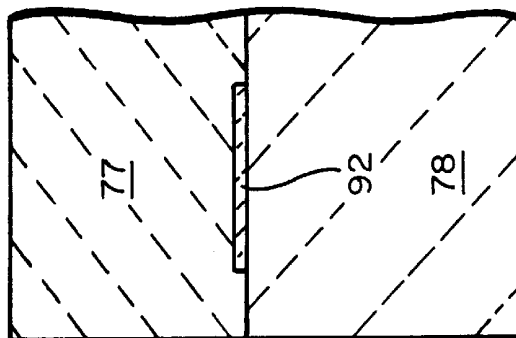
FIG-7



FIG_8



FIG_9



FIG_10

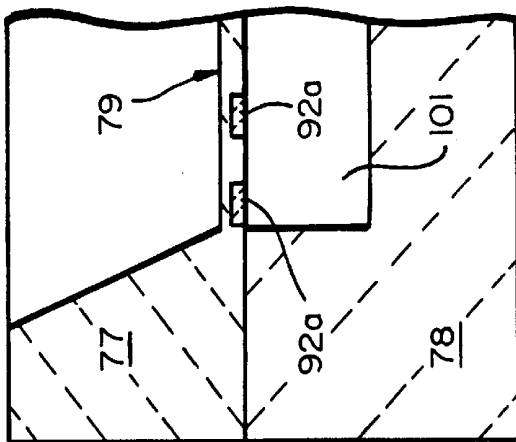


FIG-11

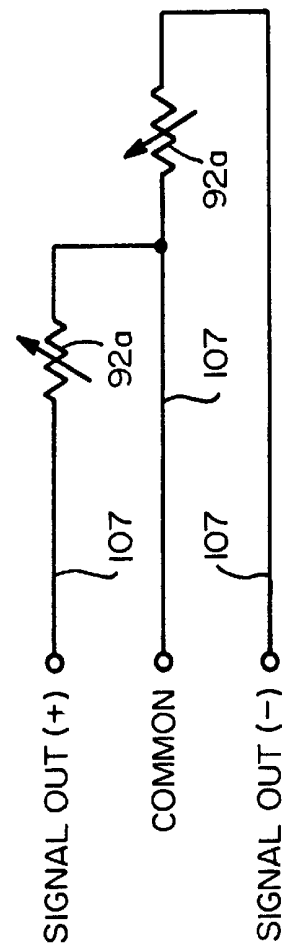
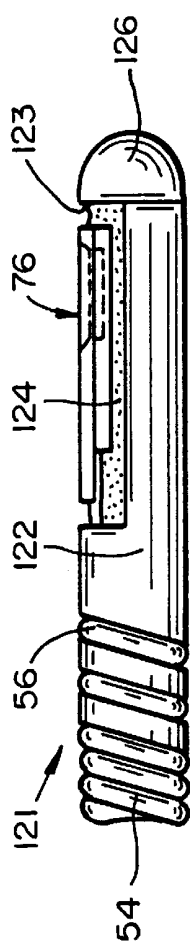
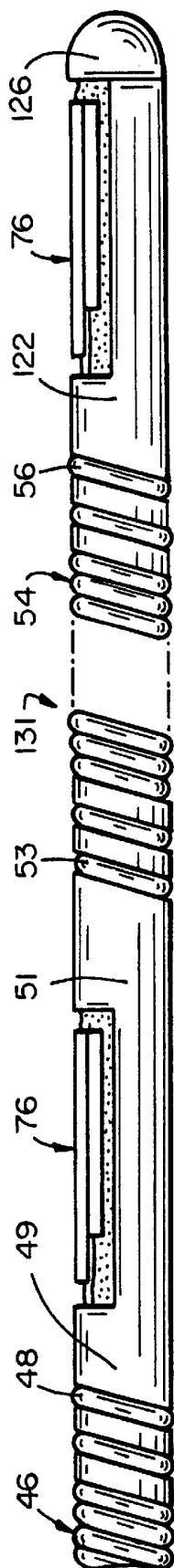


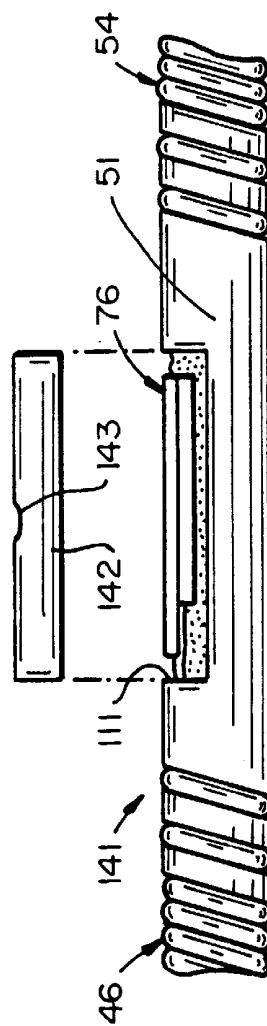
FIG-12



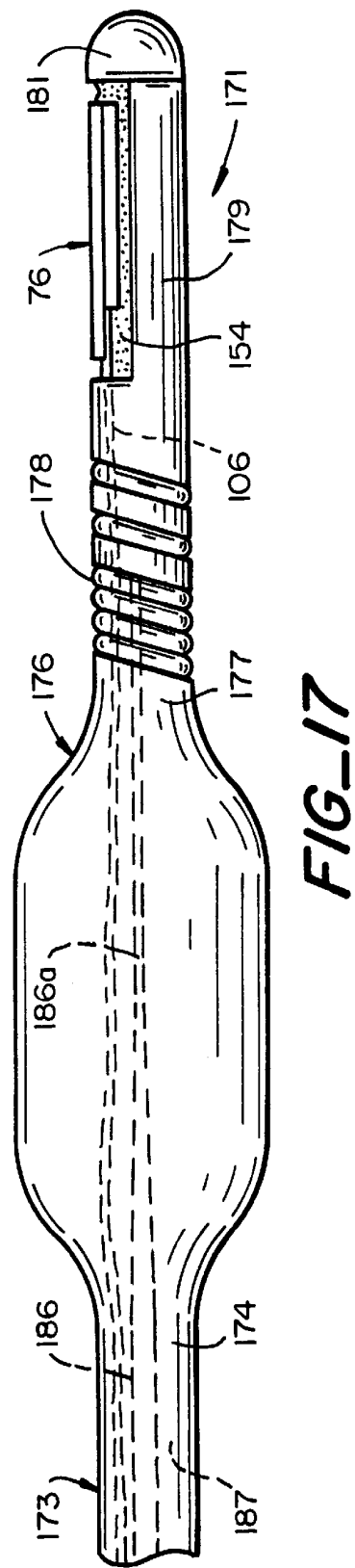
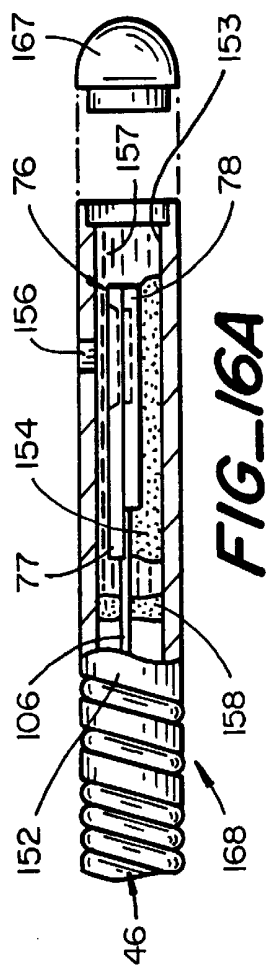
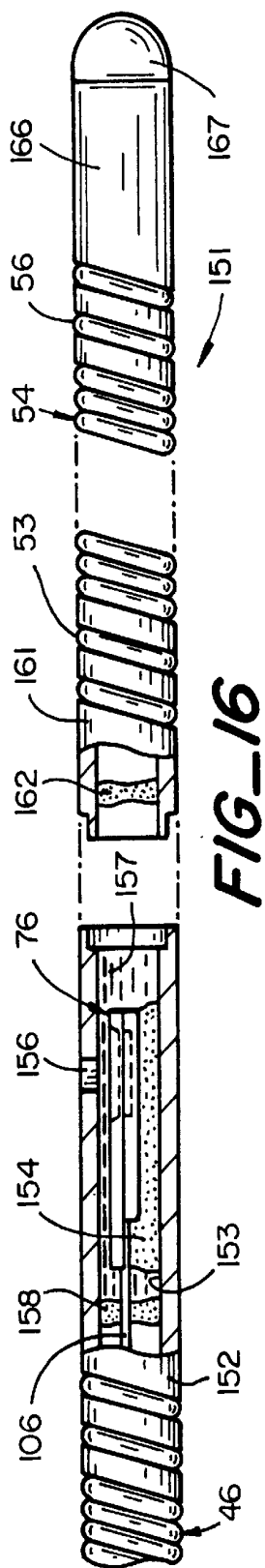
FIG_13



FIG_14



FIG_15



METHOD OF MEASURING BLOOD PRESSURE AND VELOCITY PROXIMALLY AND DISTALLY OF A STENOSIS

This application is a continuation of Ser. No. 08/912,879 filed Aug. 15, 1997, now U.S. Pat. No. 6,106,476 continuation-in-part of application Ser. No. 08/710,062 filed Sep. 9, 1996 now U.S. Pat. No. 5,715,827 which is a continuation of application Ser. No. 08/300,445 filed Sep. 2, 1994, abandoned.

This invention relates to an ultra miniature pressure sensor and guide wire and apparatus using the same and method, which is particularly suitable for making pressure measurements in coronary arteries of human beings.

It has been well known that it is desirable to make pressure measurements in vessels and particularly in coronary arteries with the advent of angioplasty. Typically in the past, such pressure measurements have been made by measuring the pressure at a proximal extremity of a lumen provided in a catheter advanced into the coronary artery of interest. However, such an approach has been less efficacious as the diameters of the catheters became smaller with the need to advance the catheter into smaller vessels. This made necessary the use of smaller lumens which gave less accurate pressure measurements and in the smallest catheters necessitated the elimination of such a pressure lumen entirely. In an attempt to overcome these difficulties, ultra miniature pressure sensors have been proposed for use on the distal extremities of catheters. However, it has not been feasible prior to the present invention to provide such ultra miniature pressure sensors which are capable of being incorporated in a guide wire for making pressure measurements in a very small arterial vessels. There is therefore a need for a new and improved ultra miniature pressure sensor and a guide wire and apparatus utilizing the same.

In general it is an object of the present invention to provide an ultra miniature pressure sensor and guide wire and apparatus utilizing the same making possible pressure and velocity measurements.

Another object of the invention is to provide a sensor which can be utilized on the distal extremity of a guide wire 0.018" or 0.014" in diameter.

Another object of the invention is to provide a sensor of the above character which is formed of a silicon chip of a small dimension which is reinforced by an additional member to provide reinforcement for the chip.

Another object of the invention is to provide a sensor of the above character in which a thin diaphragm is formed in the crystalline silicon chip.

Another object of the invention is to provide a sensor of the above character in which the reinforcing member extends for approximately 200 microns beyond the silicon diaphragm.

Another object of the invention is to provide a guide wire with the above character in which the number of conducting wires required is kept to a minimum.

Another object of the invention is to provide a guide wire and method in which simultaneous pressure and velocity measurements can be made.

Another object of the invention is to provide a guide wire of the above character in which the diaphragm area has been maximized.

Another object of the invention is to provide a guide wire with the above character in which two pressure sensors are provided on the guide wire which are spaced apart so that pressure measurements can be made on both sides of a stenosis.

Another object of the invention is to provide a guide wire of the above character in which the sensors are covered to prevent the formation of blood clots.

Another object of the invention is to provide an apparatus of the above character which includes a guide wire with an integral inflatable balloon.

Another object of the invention is to provide an apparatus of the above character in which temperature compensation can be provided.

Another object of the invention is to provide an apparatus of the above character which can be utilized in a half-bridge configuration.

Additional features and objects of the invention will appear from the following description in which the preferred embodiments are set forth in detail in conjunction with the accompanying drawings.

FIG. 1 is a schematic illustration showing use of a guide wire incorporating a pressure sensor of the present invention and apparatus utilizing the same in conjunction with a patient undergoing a catheterization procedure for diagnosis or treatment.

FIG. 2 is a side elevational view of a guide wire incorporating an ultra miniature pressure sensor of the present invention.

FIG. 3 is an enlarged side elevational view of the distal extremity of the guide wire shown in FIG. 2 and showing the pressure sensor mounted therein.

FIG. 4 is a top plan view looking along the line 4—4 of FIG. 3.

FIG. 5 is a bottom plan view looking along the line 5—5 of FIG. 3.

FIG. 6 is an isometric view of the pressure sensor shown in FIGS. 3, 4 and 5 with the lead wires connected thereto.

FIG. 7 is a side elevational view of the pressure sensor shown in FIG. 6.

FIG. 8 is a top plan view of the pressure sensor shown in FIGS. 6 and 7.

FIG. 9 is a cross-sectional view taken along the line 9—9 of FIG. 8.

FIG. 10 is a cross-sectional view taken along the line 10—10 of FIG. 8.

FIG. 11 is a cross-sectional view taken along the line 11—11 of FIG. 8.

FIG. 12, is a schematic diagram of the circuitry utilized in the pressure sensor shown in FIGS. 6—11.

FIG. 13 is a side elevational view of the distal extremity of another guide wire incorporating the pressure sensor with the sensor of the present invention being mounted in the tip housing.

FIG. 14 is a side elevational view of the distal extremity of a guide wire having first and second pressure sensors mounted in the distal extremity of the same spaced apart to permit simultaneous measurements of proximal and distal pressures with respect to a stenosis.

FIG. 15 is a partial side elevational view of another guide wire incorporating the present invention with an enclosed pressure sensor.

FIG. 16 is a side elevational view partially in section of the distal extremity of another guide wire incorporating the present invention in which the pressure sensor is enclosed in a transition housing.

FIG. 16A is a side elevational view in section showing an end-mounted pressure sensor incorporating the present invention.

FIG. 17 is a side elevational view in section of a guide wire housing a tip-mounted sensor incorporating the present invention with an integral balloon.

In general, the guide wire of the present invention having pressure sensing capabilities is comprised of a flexible elongate element having proximal and distal extremities and having a diameter of 0.018" and less. The pressure sensor is mounted on the distal extremity of a flexible elongate element. It is comprised of a crystal semiconductor material having a recess therein and forming a diaphragm bordered by a rim. A reinforcing member is bonded to the crystal and reinforces the rim of the crystal and has a cavity therein underlying the diaphragm and exposed to the diaphragm. A resistor having opposite ends is carried by the crystal and has a portion thereof overlying a portion of the diaphragm. Leads are connected to opposite ends of the resistor and extend within the flexible elongate member to the proximal extremity of the flexible elongate member.

More in particular, the guide wire **21** of the present invention having pressure measuring capabilities as shown in FIG. **1** is one that is adapted to be used in connection with a patient **22** lying on a table or a bed **23** in a cath lab of a typical hospital in which a catheterization procedure such as for diagnosis or treatment is being performed on the patient. The guide wire **21** is used with apparatus **24** which consists of a cable **26** which connects the guide wire **21** to an interface box **27**. Interface box **27** is connected by another cable **28** to a control console **29** which has incorporated as a part thereof a video screen **31** on which a waveform **32** displaying ECG measurements may be provided as well as two traces **33** and **34** displaying pressure measurements being made by the guide wire **21**.

The guide wire **21** is shown more in detail in FIG. **2** and as shown therein, the guide wire **21** can be constructed utilizing the various constructions as shown in U.S. Pat. Nos. 5,125,137; 5,163,445; 5,174,295; 5,178,159; 5,226,421; and 5,240,437. As disclosed therein, such a guide wire consists of a flexible elongate element **41** having a proximal and distal extremities **42** and **43** and which can be formed of a suitable material such as stainless steel having an outside diameter for example of 0.018" or less and having a suitable wall thickness as for example, 0.001" to 0.002" and conventionally called a "hypotube" having a length of 150–170 centimeters. Where a smaller guide wire is desired, the hypotube **41** can have an exterior diameter of 0.014" or less. Typically such a guide wire includes a core wire (not shown) of the type disclosed in the above identified patents which extends from the proximal extremity to the distal extremity of the flexible elongate element **41** to provide the desired torsional properties for guide wires (See U.S. Pat. No. 5,163,445, col. 18:40–51) to facilitate steering of the guide wire **21** in the vessel.

A coil spring **46** is provided and is formed of a suitable material such as stainless steel. It has an outside diameter of 0.018" and is formed from a wire having a diameter of 0.003". The spring **46** is provided with a proximal extremity **47** which is threaded onto the distal extremity **43** of the flexible elongate member **41**. The distal extremity **48** of the coil spring **46** is threaded onto the proximal extremity **49** of an intermediate or transition housing **51** such as disclosed in U.S. Pat. No. 5,174,295, formed of a suitable material such as stainless steel having an outside diameter of 0.018" and having a suitable wall thickness as for example, 0.001" to 0.002". The housing **51** is provided with a distal extremity **52** which has the proximal extremity **53** of a coil spring **54** threaded thereon. The coil spring **54** is formed of a highly radiopaque material such as palladium or a tungsten platinum alloy. The coil spring **46** can have a suitable length as for example 27 centimeters whereas, the coil spring **54** can have a suitable length such as 3 centimeters. The interme-

diate or transition housing **51** can have a suitable length as for example, one to five millimeters. The use of the two coils **46** and **54** on opposite ends of the housing **61** provides a very flexible floppy tip for the guide wire **21** as described in U.S. Pat. No. 5,174,295. The coil **54** is provided with a distal extremity which is threaded onto an end cap **57** also formed of a suitable material such as stainless steel and having an outside diameter of 0.018" and a wall thickness of 0.001" to 0.002". An ultrasonic transducer **58** is mounted in the end cap in a manner described in U.S. Pat. No. 5,125,137 and has conductors **61** and **62** secured to the front and rear sides of the same which extend interiorly to the proximal extremity of the flexible elongate member **41**.

A torquer **66** of the type described in U.S. Pat. No. 5,178,159 is mounted on the proximal extremity **42** of the flexible elongate member **41** for causing a rotation of a guide wire **21** when used in connection with catheterization procedures in a manner well known to those skilled in the art.

The proximal extremity **42** is also provided with a plurality of conducting sleeves (not shown) of the type disclosed in U.S. Pat. No. 5,178,159. In the present invention, one or more additional sleeves can be provided to make connection to the conductors hereinafter described. The proximal extremity **42** of the flexible elongate member is removably disposed within a housing **68** of the type described in U.S. Pat. Nos. 5,178,159, 5,348,481 and 5,358,409 that makes electrical contact with the sleeves on the proximal extremity **42** while permitting rotation of the sleeves and the flexible elongate member **41**. The housing **68** carries female receptacles (not shown) which receive the sleeves and which are connected to a cable **71** connected to a connector **72**. The connector **72** is connected to another mating connector **73** carried by the cable **26** and connected into the interface box **27**.

The portion of the guide wire **21** therefore described is substantially conventional. In accordance with the present invention it is provided with a pressure measuring capability in the form of a pressure sensor assembly **76** which is mounted within the intermediate or transition housing **51**. The pressure sensor assembly **76** consists of a diaphragm structure **77** supported by a base plate **78**. The diaphragm structure **77** is formed of suitable materials such as "n" type or "p" type 100 oriented silicon with a resistivity of approximately 6–8 ohm-centimeters. The diaphragm structure **77** is a die made from such a wafer. In accordance with the present invention, the die has a suitable length, as for example, 1050 microns and for a 0.014" guide wire has a width of 250 microns and for a 0.018" guide wire has a width of between 250 and 350 microns. It can have a suitable thickness, as for example, 50 microns. A rectangular diaphragm **79** is formed in the diaphragm structure **77** of a suitable thickness, as for example, 2.5 microns and having dimensions such as a length of 350 microns. The diaphragm **79** has first and second or top and bottom surfaces **80** and **81**. The diaphragm is formed by utilization of conventional masking and crystal etching techniques which create a die with two parallel sloping endwalls **82** and two parallel sidewalls **83** extending at right angles to the end walls **82** leading down to the top surface **80** of the diaphragm **79** to form a well **84**. As hereinafter explained, the diaphragm **79** is made relatively wide in comparison to the diaphragm structure **77** so that what remains is a relatively narrow rim **86** formed by side portions **87** and **88** and an end portion **89**. As can be seen from FIGS. **6**, **7** and **8**, the diaphragm **79** is located at or near one end of the diaphragm structure or die **77**. It has been found that it is desirable to provide a rectangular geometry for the diaphragm **79** rather than a square geometry in order

to obtain the highest possible sensitivity for pressure measurements. For example, it has been found that the rectangular diaphragm provides approximately 1.5 times more sensitivity than does a square diaphragm for the same diaphragm thickness and width.

In etching the well **84** to form the diaphragm **81**, an impurity can be implanted into the backside of the diaphragm structure **77** before the etching process is commenced so that etching will stop at the desired depth, as for example, within 2 to 3 microns of the bottom surface **81** to provide a diaphragm **79** having a thickness ranging from 2 to 5 microns, and for example, the preferred thickness of 2.5 microns. Because the rim **86** provided on the diaphragm structure **77** surrounding the rectangular diaphragm **79** is relatively thin, the base plate **78** provides support for this rim to provide the necessary strength for the pressure sensor **76**.

In order to obtain adequate performance characteristics such as sensitivity in the miniaturized pressure sensor assembly **76** hereinbefore described, it has been found desirable to have as much of the width of diaphragm structure **77** as possible be occupied by the diaphragm **79** and at the same time to minimize the portion of the diaphragm structure **77** occupied by the rim. In order to achieve a diaphragm width ratio of at least 0.45 to 0.9 with respect to the width of the diaphragm **79** to the width of the structure **77** and therefore to obtain the largest diaphragm possible in the diaphragm structure **77**, diaphragm **79** is made relatively large compared to rim **86**. With current manufacturing technology, it has been found feasible to have a width of rim **86** of 40 microns, which provides for a diaphragm **79** of 170 microns in a 250 micron-wide diaphragm structure **77** to provide a diaphragm width ratio of 0.68. In a larger diaphragm structure such as 350 microns wide, the pressure sensor assembly **76** can be made stronger by increasing the rim width to 90 microns. Alternatively, it can be made more sensitive by increasing the diaphragm width up to 270 microns. This results in a diaphragm width ratio for a 350 micron-wide device of between 0.49 and 0.77, depending on what combination of sensitivity and strength is desired.

Prior to or after the formation of the rectangular diaphragm **79**, a plurality of V-shaped recesses or grooves **91** are formed in the diaphragm structure **77** on the end opposite the end at which the diaphragm **79** is located and on the side opposite the side in which the well **84** is formed. These V-shaped recesses **91** also can be formed in a conventional manner by the use of a conventional etch. It should be appreciated that if desired, the etching can be stopped so that the recesses formed are short of a complete V. By way of example, if the etching for the V-shaped recess was stopped at a depth of 12 microns, the bottom of the substantially V-shaped recess or trench **91** would be approximately 8 microns wide.

After the V-shaped or substantially V-shaped recesses have been formed, a P+ diffusion utilizing a suitable material such as boron can be carried out to create a V-shaped region **92** (in the structure **77**) which underlies the V-shaped recess **91**. Utilizing suitable masking a common layer **93** of a suitable material such as chromium is sputtered into the V-shaped recess **91** to a suitable thickness as for example, 300 Angstroms followed by a layer **94** of a suitable material such as gold of a suitable thickness as for example 3000 Angstroms. The layers **93** and **94** overlie the bottom surface **81** to form pads **96** thereon. In depositing the gold just short of the leftmost extremity of the V-shaped recess as viewed in FIG. 8 in order to minimize the likelihood of lead-to-lead shorting during the dicing operation when a wafer is sawed up into individual sensor chips.

By way of example, the spacing between V-grooves **91** from center to center can be 75 microns with the V-groove having a width of 25 microns and having a typical depth of 18 microns. The metal pads **96** formed by the chromium and gold layers **93** and **94** can have a suitable width as for example, 50 microns with the overlap on each side being approximately 12.5 microns to provide a spacing of approximately 25 microns between adjacent V-shaped pads **96**. The bottom of the V-shaped groove can have a total length of approximately 250 microns.

The regions **92** formed from the P+ diffusion have patterns that extend to the right from the three V-shaped recesses **91** as viewed in FIG. 8 for a distance so that they underlie the approximate midpoint of the diaphragm **81** on opposite sides to provide generally U-shaped portions or resistors **92a** which are located on the diaphragm in areas of a maximum stress to provide maximum sensitivity to pressure changes. The resistors **92a** are provided with opposite ends, one end being connected to one each of the V-grooves and the other end being connected to the center or common V-groove. Contact is made to these P+ diffused regions by the chromium and gold layers **93** and **94** hereinbefore described.

The base plate **78** can be formed of a suitable material such as Pyrex supplied by Corning Glassworks and can have the same width as the diaphragm structure **77** but has a length which is less than the length of the diaphragm structure **77** so that the V-shaped grooves **91** are exposed on the underside of the diaphragm structure **77** as shown in FIG. 6. It also can have a suitable length such as 850 microns. It is provided with a rectangular recess or cavity **101** having substantially the same size as the diaphragm **79**. It can be etched into the Pyrex by suitable means such as a conventional etching process utilizing hydrochloric acid. After the etching has been completed to form the rectangular recess **101** it is bonded to the lower surface of the diaphragm structure **77** to form a hermetic seal with respect to the same so that the cavity **101** underlies the diaphragm **79** and is exposed to the bottom surface **81** of the diaphragm **79**. The cavity **101** below the diaphragm **79** serves as a reference pressure chamber and can be filled with a suitable fluid. For example, it can be filled with air to half an atmosphere to provide a partial vacuum. Alternatively, the cavity **101** can be filled to one atmosphere or it can be completely evacuated.

A trifilar lead structure **106** is connected to the rectangular diaphragm structure **77**. It has insulated copper leads **107** of a suitable diameter as for example 48AWG soldered into place to the V-shaped recesses **91** so that the leads **107** extend outwardly therefrom and lie in a plane parallel to the plane of the diaphragm structure **77**. The trifilar lead construction **106** provides insulation around each lead and in addition there is provided additional insulation which surrounds the leads and which interconnects the leads into a single unit which can be readily extended through the hypotube forming the flexible elongate member **41**.

The pressure sensor assembly **76** is mounted within a cutout **111** provided in the transition housing **51** and secured therein by suitable means such as an epoxy **112** so that the outer surface of the pressure sensor assembly **76** is generally flush with the outer surface of the transition housing **51** (see FIG. 3) and so that the diaphragm **79** is exposed to ambient and the leads **106** extend through the flexible elongate member **41** to the proximal extremity **42** of the same where they are connected to the sleeves (not shown) carried by the proximal extremity **42** disposed within the housing **68**. Also, the conductors **61** and **62** of the velocity sensing transducer

58 are connected to two of such sleeves (not shown) provided on the proximal extremity 42.

A schematic of the wiring for the pressure sensor assembly 76 is shown in FIG. 12. The two generally U-shaped portions 92a on opposite sides of the diaphragm 79 are represented as resistors and are connected to the three leads 107 in the manner shown. One of the first of the outside leads 107 is "SIGNAL OUT" (+) and the second or other outside lead is "SIGNAL OUT" (-) and the third or middle lead is a common lead as shown. This pattern makes it possible to not cross leads and has the third lead going up the middle or center of the die or the diaphragm structure 77. It can be seen that the two resistors 92a connected as shown form a half bridge one of the resistors responds positively to pressure change and the other resistor responds negatively to a pressure change. Thus, as a pressure is supplied to the diaphragm 79, one resistor increases in value and the other resistor decreases in value to provide a voltage change. By applying the same current to both resistors at the same time, temperature effects can be measured because temperature change will affect both of the resistors in the same way so that the pressure measurements can be compensated for any changes in temperature which are sensed by the resistors 92a. The changes in resistivity caused by the temperature changes in the resistors will cancel each other out because of the half bridge configuration used. In connection with FIG. 12 it can be seen that with the use of three leads it is possible to obtain temperature compensation by utilizing a half-bridge configuration for the pressure sensor. Alternatively, a more precise temperature compensation can be provided by directly measuring the two resistances, and then solving the mathematical equations which relate temperature and pressure to the two sensor resistances.

Operation and use of the guide wire 21 in performing a catheterization procedure such as angioplasty may now be briefly described as follows: Let it be assumed that a guiding catheter (not shown) has been introduced into the femoral artery of the patient 22 shown in FIG. 1 with the distal extremity near the desired location in the heart in which it is desired to perform an angioplasty. The guide wire 21 of the present invention is inserted into the guiding catheter. At the time that its distal extremity is in close proximity to the distal extremity of the guiding catheter, the pressure output signal from the guide wire is compared with that of the guiding catheter assuming that the guide wire is provided with pressure sensing capabilities. If there is a difference between the two pressure measurements, the pressure measurement from the guide wire 21 is equalized with that from the guiding catheter at the control console 29. The distal extremity of the guide wire 21 is then advanced so that it is proximal of the stenosis to be treated at which time a pressure measurement is made. After this pressure measurement has been recorded, the distal extremity of the guide wire is then advanced through the stenosis and another pressure measurement made to determine whether the stenosis is severe enough to require treatment by angioplasty. Alternatively, the distal extremity of guide wire 21 can be immediately advanced to the distal side of the stenosis rather than making a pressure measurement proximal of the stenosis and thereafter comparing the pressure measurement on the distal extremity being measured by the guide wire 21 with the pressure measurement being provided proximal of the stenosis by the guiding catheter. If it is determined that the stenosis causes a partial occlusion which is severe enough to warrant use of an angioplasty procedure, an angioplasty catheter having a balloon thereon (not shown) can be advanced over the guide wire 21 and advanced into

the stenosis to dilate the stenosis. After dilation has occurred, the angioplasty balloon can be withdrawn from the stenosis and pressure measurements can be made proximal and distal of the stenosis to ascertain the effect of the angioplastic treatment. If the pressure measurements indicate that the original dilation by the angioplasty balloon has been inadequate, another balloon catheter as for example, one having a balloon of a greater diameter can then be positioned over the guide wire 21 by utilizing an exchange wire if appropriate. The larger angioplasty catheter can be advanced through the stenosis and inflated to again dilate the stenosis to a larger size after which it can be withdrawn. Thereafter, pressure measurements proximal and distal of the stenosis can again be made to ascertain whether or not the second dilation which has been performed is adequate. The decisions to be made in connection with such procedures can be readily made by use of the control console 29 by observing the traces 33 and 34 on the video monitor 31.

It also should be appreciated that at the same time Doppler velocity measurements can be made by the transducer 58. That information can be used in connection with the pressure measurements to ascertain the need for performing the angioplasty procedure or for determining the efficacy of the angioplasty procedure performed. Because of the very small diameters of the guide wires as for example, 0.018" or 0.014", it is possible to utilize the guide wire 21 of the present invention with very small coronary vessels in the heart. In connection with the leads from the Doppler transducer 58 it should be appreciated that if desired some of the conductors provided for the Doppler ultrasound transducer can be shared with the wires or conductors provided for the pressure sensor assembly 76. Thus, two of the wires for the pressure sensor can be utilized for the Doppler transducer because the pressure sensor operates at DC or up to a few hundred Hz or KHz whereas the Doppler sensor operates at 10 MHz and above. These frequency ranges can be readily separated by one skilled in the art by using simple filters and the appropriate circuitry.

In connection with the present invention it should be appreciated that rather than bonding the leads 107 into the V-grooves or V-shaped recesses 91, the Pyrex base plate 78 can be formed so it has the same length as the diaphragm structure 77. V-shaped or U-shaped grooves can be formed in the base plate underlying the V-shaped grooves to in effect form little tunnels which can be utilized for receiving the wires 107 and for them to be soldered therein. Such a construction aids in the placement of wires which are of the very small diameter, as for example, 1 mil.

Another embodiment of a guide wire 121 incorporating the present invention is shown in FIG. 13. In the guide wire 121, pressure sensor assembly 76 is mounted in a tip housing 122. The tip housing 122 can be substituted at the end cap 57 and threaded into the distal extremity 56 of the coil 54. The tip housing 122 can be formed of a suitable material such as stainless steel having an outside diameter of 0.018" and a wall thickness of 0.001" to 0.002". The sensor assembly 76 can be of the type hereinbefore described and can be mounted in a cutout 123 provided in the tip housing 122 much in the same manner as the sensor assembly 76 was mounted in the cutout 111 in the transition housing 51 such as by use of an epoxy 124. An hemispherical end cap 126 formed of a radiopaque material such as palladium or tungsten platinum alloy can be mounted on the distal extremity of the tip housing 122. Alternatively, the end cap 126 can be formed of a non-radiopaque material such as epoxy or silicone rubber.

Thus it can be seen with the embodiment of the guide wire 121 shown in FIG. 13, the guide wire 121 can be

utilized in the same manner as the guide wire 21 hereinbefore described with the exception of it cannot be used for making velocity measurements because that capability has been removed from the guide wire 121.

Another guide wire 131 incorporating the present invention is shown in FIG. 14 in which two pressure sensors 76 have been provided. The sensors 76 have been spaced apart a suitable distance as for example, 3 centimeters with one of the pressure sensors being mounted in the transition housing 51 and the other pressure sensor being mounted in a tip housing 122 of the type shown in FIG. 13. With such an arrangement, it can be seen that the distal extremity of the guide wire 131 can be advanced across a stenosis in a vessel with the pressure sensor 76 mounted in the tip housing being distal of the stenosis to measure distal pressure and the pressure sensor 76 in the transition housing 51 being proximal of the stenosis to measure proximal pressure. Thus, it can be seen that it is possible to measure simultaneously the distal pressure and the proximal pressure with respect to a stenosis in a vessel. This may give more accurate measurements than utilizing the proximal pressure being sensed by the guiding catheter.

When using two pressure sensors 76 in the same guide wire as shown in FIG. 14, it is possible to utilize the same common wire for both of the transducers, thus making it necessary to provide only five wires rather than six wires for the two pressure sensors.

Still another guide wire 141 incorporating the present invention is shown in FIG. 15 in which a cover 142 is provided for covering the pressure sensor assembly 76 provided in the transition housing 51. The cover is elongate and extends the length of the cutout 111 and is arcuate in cross-section so that it conforms to the conformation of the transition housing 51. The cover 142 can be secured in place by a suitable means such as an adhesive. The cover 142 overlying the pressure sensor assembly 76 is provided with a pin hole 143 which immediately overlies the diaphragm 79. The pin hole 143 can be of a suitable size as for example 2-5 mils in and preferably 3 mils in diameter. The cover 142 serves to prevent the large opening provided by the cutout 111 from collecting blood which could possibly clot. The cover 142 also serves to protect the sensor 76 from damage. It also prevents the sensor 76 from being broken loose during use of the guide wire 141. It should be appreciated that if desired, the volume beneath the cover 142 can be filled with viscous fluid such as oil which can be utilized for transmitting pressure from the pin hole 143 to the diaphragm 81. With a small size pin hole 143, the viscous fluid provided would not have a tendency to bleed out of the transition housing 51. The viscous fluid would be held in place because of the surface tension of the fluid. Because there is a very short distance between the pin hole 143 and the diaphragm 79, there would be very little tendency for the viscous fluid to damp any pressure signal transmitted from the blood in which the guide wire 141 is disposed to the diaphragm.

Another guide wire 151 incorporating the present invention is shown in FIG. 16 having a transition housing 152 formed of a suitable material such as stainless steel and having an OD of 0.018" or less. A pressure sensor assembly 76 of the type hereinbefore described is mounted within the bore 153 of the transition housing 152 and is secured therein by mounting the same in an epoxy 154 while leaving the area immediately above the diaphragm 79 exposed to a pin hole 156 provided in the transition housing 152. The space overlying the diaphragm 81 exposed to the pin hole 156 can be filled with a viscous fluid 157 such as oil. The viscous fluid 157 can be retained within the desired location by a

barrier 158 formed on the proximal side of the pressure sensor 76 having the trifilar lead structure 106 extending therethrough, in sealing engagement therewith. To seal the other end of the bore 153, an intermediate end cap 161 can be provided which is provided with a barrier 182 extending thereacross to seal the bore 153. The intermediate end cap 161 can be bonded to the transition housing 152 by a suitable means such as an adhesive (not shown). The coil 54 can be threaded onto the intermediate end cap 161 and can be threaded onto a tip housing 166 that carries a rounded hemispherical tip 167. With such a construction it can be seen that the pressure sensor assembly 76 is protected within the transition housing 152.

In FIG. 16A a guide wire 168 is shown which is very similar to the guide wire 151 with the exception that the housing 152 has been provided on the distal extremity of the coil 46 with the tip 167 directly mounted on the housing 152 for closing the bore 153.

In FIG. 17 there is shown another embodiment of a guide wire 171 incorporating the present invention which has an integral balloon carried thereby. A guide wire with an integral balloon is described in U.S. Pat. No. 5,226,421. The guide wire 171 consists of a flexible elongate tubular member 173 in a manner formed of a suitable material such as plastic which is provided with a distal extremity 174. An inflatable balloon 176 is secured to the distal extremity 174 of the flexible elongate member 173 in a manner well known to those skilled in the art. Such a balloon can be formed integral with the distal extremity and can be formed of the same material as the flexible elongate tubular member 173. Alternatively, it can be formed of a different material or the same material and be formed as a separate part and secured to the distal extremity 174 by suitable means such as adhesive.

The balloon 176 is provided with a distal extremity which is closed and which is secured to the proximal extremity of a coil spring 178 formed of a radiopaque material such as a palladium or tungsten platinum alloy threaded onto a tip housing 179. The tip housing 179 can be formed in a manner similar to the tip housing 122 shown in FIG. 13 having a pressure sensor 76 mounted therein and carrying an end cap 181. The trifilar leads 106 connected to the sensor 76 extend through the coil 178 and through the balloon 176 and through the flexible elongate tubular member 172 to the proximal extremity thereof. A core wire 186 formed of a suitable material such as stainless steel is provided in the flexible elongate member 173 and can be provided with a diameter such as disclosed in U.S. Pat. No. 5,226,421. The core wire 186 is provided with a tapered portion 186a extending through the balloon which has a distal extremity secured to the housing 179 by a suitable means such as the epoxy utilized for mounting the sensor 76 within the housing. The flexible elongate tubular member 172 is provided with a balloon inflation lumen 187 which can be used for inflating and deflating the balloon 176.

The guide wire 171 with an integral balloon 171 can be utilized in a manner similar to that hereinbefore described for the other guide wires. Rather than deploying a separate catheter with a balloon thereon over the guide wire, the guide wire 171 itself carries the balloon 176 which can be inflated to dilate the stenosis after the proximal and distal pressure measurements have been made by the tip mounted sensor 76. After the balloon 176 has been deflated, the pressure measurement can be made to ascertain the pressure in the distal extremity after dilation has occurred. If necessary, the balloon 176 can be re-inflated to perform another dilation of the stenosis to obtain improved blood flow through the stenosis.

After an appropriate dilation has occurred, the guide wire 171 with integral balloon can be removed in a conventional manner. The angioplasty procedure can then be completed in a conventional manner.

From the foregoing, it can be seen that there has been provided an ultra miniature pressure sensor which can be utilized on guide wires having a diameter of 0.018" and less which can be utilized for making accurate measurements proximal and distal of a stenosis in the coronary vessel. This is made possible because of the small size of the pressure sensor incorporated into the distal extremity of the guide wire. In addition to sensing pressure, flow velocity can also be obtained by the use of a distally mounted velocity transducer provided on the same guide wire as on which the pressure sensor is mounted. Alternatively, additional first and second pressure sensors can be provided on the distal extremity of a guide wire so that pressure measurements can be made simultaneously, proximally and distally of the stenosis. The pressure sensor is constructed in such a manner so that it can be readily incorporated within the confines of a small guide wire as for example, 0.018" and less. It can be constructed to avoid a large opening in the distal extremity of the guide wire to inhibit or prevent the formation of clots. The pressure sensor also can be protected so that it cannot be readily damaged or broken loose. In addition, where desired, the guide wire can be provided with an integrally mounted balloon on its distal extremity so that the guide wire can be utilized for performing an angioplasty procedure while at the same time facilitating the making of pressure measurements, proximal and distal of the stenosis being treated.

What is claimed:

1. A method of measuring blood pressure and velocity proximally and distally of a stenosis in a vessel carrying blood, comprising the steps of:

introducing a guide wire carrying a solid state pressure sensor and a velocity transducer into the vessel, the guide wire having a core wire extending from a proximal region to a distal region of the guide wire, the pressure sensor and the velocity transducer disposed on a distal region of the guide wire,

advancing the guide wire to position the pressure sensor and the velocity transducer proximally and distally of the stenosis, and

measuring blood pressure and velocity proximally and distally of the stenosis with the pressure sensor and the velocity transducer carried by the guide wire.

2. The method of claim 1 wherein the pressure sensor operates at a relatively low frequency and the velocity transducer operates at a relatively high frequency.

3. The method of claim 2 wherein the velocity transducer is operated at a frequency on the order of 10 MHz.

4. The method of claim 1 wherein the pressure sensor and velocity transducer are coupled to a common set of conductors.

5. The method of claim 1 wherein the pressure sensor and velocity transducer are coupled to a common set of conductors.

6. The method of claim 1 wherein the step of measuring blood pressure and velocity comprises the steps of:

first measuring the blood pressure and velocity proximally of the stenosis, and

subsequently measuring the blood pressure and velocity distally of the stenosis.

7. The method of claim 1 wherein the step of measuring blood pressure and velocity comprises the steps of:

first measuring the blood pressure and velocity distally of the stenosis, and

subsequently measuring the blood pressure and velocity proximally of the stenosis.

8. The method of claim 1 further comprising the steps of: advancing an angioplasty catheter having a balloon thereon over the guide wire to the location of the stenosis, and

dilating the stenosis with a balloon.

9. The method of claim 1 further comprising the step of dilating a balloon carried by the guide wire at the location of the stenosis.

10. A method of measuring blood pressure proximally and distally of a stenosis in a vessel carrying blood, comprising the steps of:

advancing a guide wire having a core wire extending from a proximal region to a distal region of the guide wire and carrying a solid state pressure sensor disposed on a distal region of the guide wire within the vessel to position the pressure sensor relative to the stenosis, and measuring blood pressure proximally and distally of the stenosis with the pressure sensor, wherein the blood pressure is measured by monitoring changes in a pair of resistive elements which respond oppositely to changes in pressure but are affected in a similar manner by changes in temperature.

11. A method of measuring blood pressure proximally and distally of a stenosis in a vessel carrying blood, comprising the steps of:

introducing a guide wire carrying a first pressure sensor into the vessel,

introducing a catheter carrying a second pressure sensor into the vessel over the guide wire,

advancing the guide wire within the vessel to position the first sensor distally of the stenosis,

advancing the catheter within the vessel to position the second sensor proximally of the stenosis,

measuring blood pressure distally of the stenosis with the first sensor, and

measuring blood pressure proximally of the stenosis with the second sensor.

12. The method of claim 11 including the steps of taking pressure measurements with the two sensors proximal of the stenosis, and equalizing the two measurements before advancing the guide wire to position the first sensor distally of the stenosis.

13. The method of claim 11 wherein the blood pressure is measured by monitoring changes in a pair of resistive elements which respond oppositely to changes in pressure but are affected in a similar manner by changes in temperature.

14. The method of claim 11 wherein the first pressure sensor is a solid state sensor.

15. A method of determining whether an angioplasty procedure is appropriate for treatment of a stenosis in a vessel carrying blood, comprising the steps of:

advancing a guide wire having a core wire extending from a proximal region to a distal region of the guide wire with a solid state pressure sensor and a velocity transducer disposed on a distal region of the guide wire into the vessel so that the pressure sensor and the velocity transducer are positioned proximally of the stenosis, measuring the pressure and the velocity of the blood in the vessel on the proximal side of the stenosis,

advancing the guide wire through the stenosis so that the pressure sensor and the velocity transducer are positioned distally of the stenosis,

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measuring the pressure and the velocity of the blood in the vessel on the distal side of the stenosis, and

determining whether an angioplasty procedure is appropriate for treatment of the stenosis on the basis of the pressure and velocity measurements.

16. The method of claim 15, wherein the pressure sensor operates a relatively low frequency and the velocity transducer operate at a relatively high frequency.

17. The method of claim 15 wherein the velocity transducer operates at approximately 10 MHz.

18. The method of claim 15 wherein the pressure sensor and velocity transducer are coupled to a common set of conductors.

19. A method of measuring blood pressure and velocity proximally and distally of a stenosis in a vessel carrying blood, comprising the steps of:

providing a guide wire having both a pressure sensor and a velocity sensor disposed on a distal region of the guide wire, the guide wire having a core wire extending from a proximal region to a distal region of the guide wire,

introducing the guide wire into the vessel,

advancing the guide wire to position the pressure sensor and the velocity transducer proximally and distally of the stenosis, and

measuring blood pressure and velocity proximally and distally of the stenosis with the pressure sensor and the velocity sensor.

20. The method according to claim 19 wherein the pressure sensor is a solid state pressure sensor.

21. The method according to claim 19 wherein the velocity sensor is a transducer.

22. The method of claim 19 further comprising the step of determining whether an angioplasty procedure is appropri-

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ate for treatment of the stenosis on the basis of the pressure and velocity measurements.

23. The method of claim 19 wherein the step of measuring blood pressure and velocity comprises the steps of:

5 first measuring the blood and velocity proximally of the stenosis, and

subsequently measuring the blood pressure and velocity distally of the stenosis.

24. The method of claim 19 wherein the step of measuring blood pressure and velocity comprises the steps of:

10 first measuring the blood pressure and velocity distally of the stenosis, and

subsequently measuring the blood pressure and velocity proximally of the stenosis.

25. The method of claim 19 further comprising the steps of:

advancing an angioplasty catheter having a balloon thereon over the guide wire to the location of the stenosis, and

20 dilating the stenosis with a balloon.

26. The method of claim 19 further comprising the step of dilating a balloon carried by the guide wire at the location of the stenosis.

27. The method of claim 19, wherein the step of advancing the guide wire comprises the steps of positioning both the pressure sensor and the velocity transducer proximally of the stenosis and positioning both the pressure and velocity transducer distally of the stenosis.

28. The method of claim 27, wherein the step of measuring blood pressure and velocity comprises the steps of measuring both blood pressure and velocity proximally of the stenosis and measuring both blood pressure and velocity distally of the stenosis.

* * * * *

UNITED STATES PATENT AND TRADEMARK OFFICE
CERTIFICATE OF CORRECTION

PATENT NO. : 6,767,327 B1
APPLICATION NO. : 09/644111
DATED : August 21, 2000
INVENTOR(S) : Paul D. Corl, Robert Z. Obara and John E. Ortiz

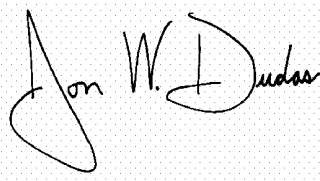
Page 1 of 1

It is certified that error appears in the above-identified patent and that said Letters Patent is hereby corrected as shown below:

At column 13, line 25 (Claim 19), please replace "transducer" with --sensor--.

Signed and Sealed this

Ninth Day of January, 2007

A handwritten signature in black ink on a light gray dotted background. The signature is written in a cursive style and reads "Jon W. Dudas".

JON W. DUDAS
Director of the United States Patent and Trademark Office

UNITED STATES PATENT AND TRADEMARK OFFICE
CERTIFICATE OF CORRECTION

PATENT NO. : 6,767,327 B1
APPLICATION NO. : 09/644111
DATED : July 27, 2004
INVENTOR(S) : Paul D. Corl, Robert Z. Obara and John E. Ortiz

Page 1 of 1

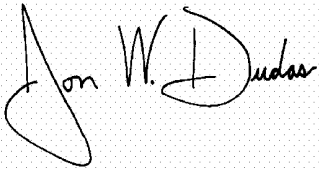
It is certified that error appears in the above-identified patent and that said Letters Patent is hereby corrected as shown below:

At column 13, line 25 (Claim 19), please replace "transducer" with --sensor--.

This certificate supersedes Certificate of Correction issued January 9, 2007.

Signed and Sealed this

Sixth Day of February, 2007

A handwritten signature in black ink on a light gray dotted background. The signature is written in a cursive style and reads "Jon W. Dudas".

JON W. DUDAS
Director of the United States Patent and Trademark Office

专利名称(译)	测量狭窄的近端和远端的血压和速度的方法		
公开(公告)号	US6767327	公开(公告)日	2004-07-27
申请号	US09/644111	申请日	2000-08-21
[标]申请(专利权)人(译)	Volcano治疗		
申请(专利权)人(译)	Volcano治疗, INC.		
当前申请(专利权)人(译)	Volcano治疗, INC.		
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发明人	CORL, PAUL D. OBARA, ROBERT Z. ORTIZ, JOHN E.		
IPC分类号	A61B5/0215 G01L9/00 A61F2/958 A61M25/00 A61M25/09 A61B5/00		
CPC分类号	A61B5/0215 A61B5/6851 A61M25/09 G01L9/0054 G01L19/0084 G01L19/141 G01L19/147 A61M25/10 A61M25/0002 A61M25/09008 A61M25/09083 A61B8/06 A61B8/12 G01L19/149		
外部链接	Espacenet USPTO		

摘要(译)

一种测量携带血液的血管狭窄的近端和远端的血压和速度的方法包括以下步骤：提供具有压力传感器和设置在导丝远端区域上的速度传感器的导丝，引入导丝进入血管，推进导丝，将压力传感器和速度传感器定位在狭窄的近端和远端，并用压力传感器和速度传感器测量狭窄的近端和远端的血压和速度。

