



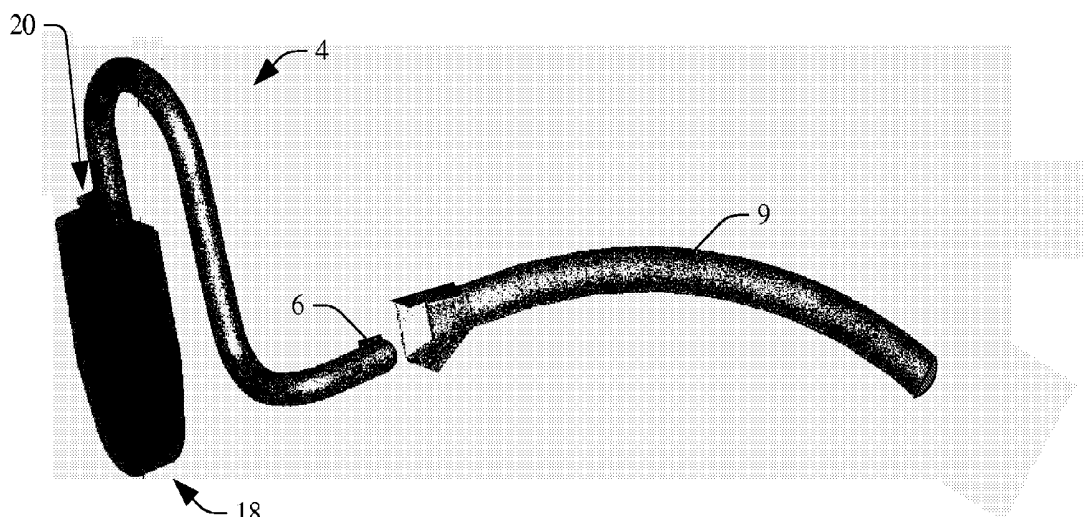
US 20090069645A1

(19) **United States**(12) **Patent Application Publication**  
**Nielsen et al.**(10) **Pub. No.: US 2009/0069645 A1**(43) **Pub. Date: Mar. 12, 2009**(54) **SIZING AND POSITIONING TECHNOLOGY  
FOR AN IN-THE-EAR  
MULTI-MEASUREMENT SENSOR TO  
ENABLE NIBP CALCULATION****Related U.S. Application Data**(60) Provisional application No. 60/695,725, filed on Jun.  
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Mercerville, NJ (US)**Publication Classification**(51) **Int. Cl.**  
**A61B 5/00** (2006.01)(52) **U.S. Cl.** ..... **600/301**

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(NL)(21) Appl. No.: **11/995,006**(22) PCT Filed: **Jun. 13, 2006**(86) PCT No.: **PCT/IB2006/051892**§ 371 (c)(1),  
(2), (4) Date:**Nov. 11, 2008**(57) **ABSTRACT**

An in-the-ear (ITE) physiological measurement device (2) includes a structure (4) formed for easy insertion into multiple shaped and sized ear canals. An inflatable balloon (6) surrounds an end portion of the structure (4) to be positioned in the ear. Optionally, a mushroom shaped tip (22) is connected with an end of the structure (4) and carries a plurality of sensors (8). Inflation of the balloon (6) expands the tip (22) radially to position the sensors (8) proximate to vascular tissue within the ear canal. Once suitably positioned, the one or more sensors (8) sense physiological signals from the vascular tissue and bone structure.



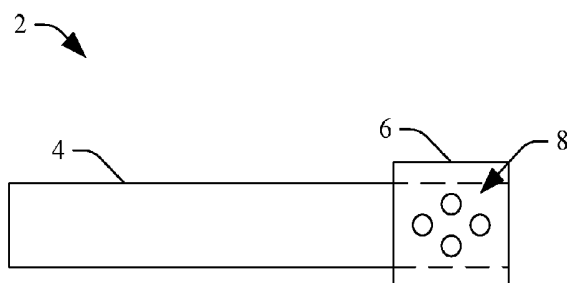


FIGURE 1

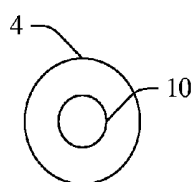


FIGURE 2



FIGURE 3

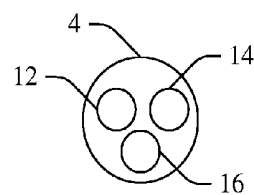


FIGURE 4

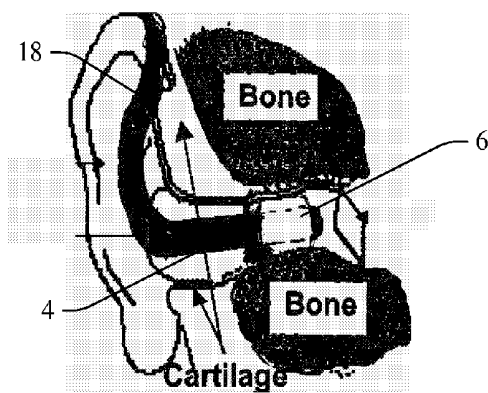


FIGURE 5

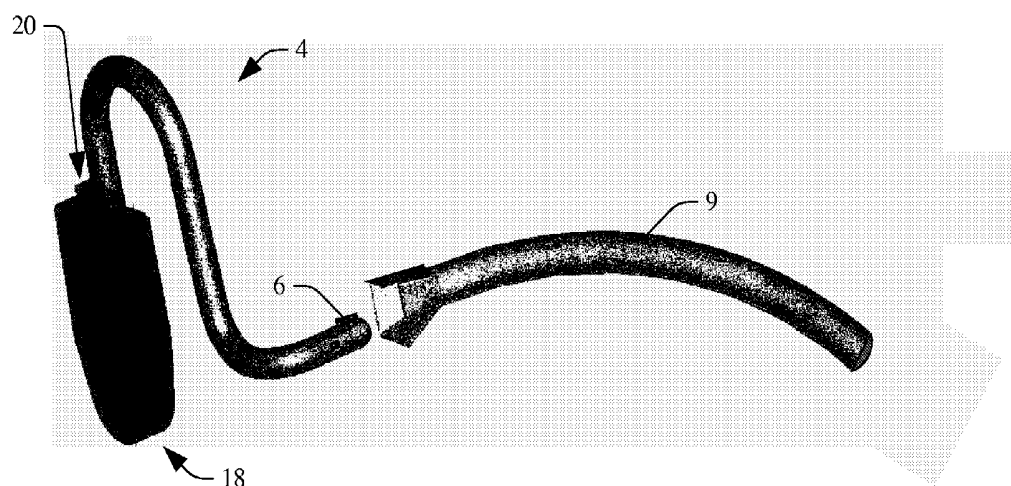


FIGURE 6

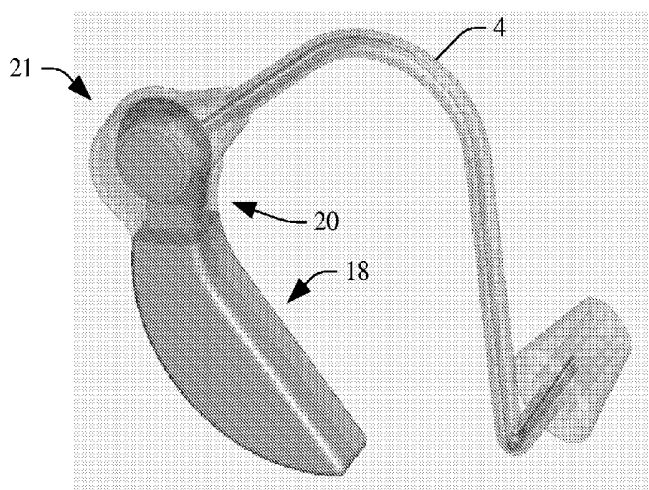


FIGURE 7

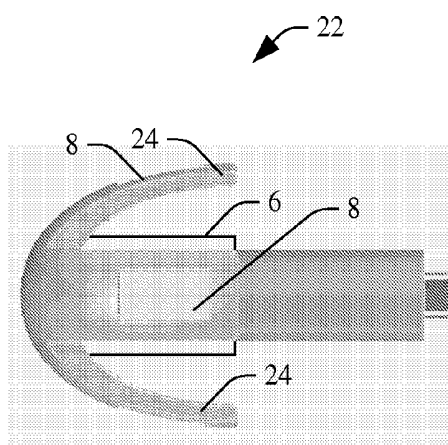


FIGURE 8

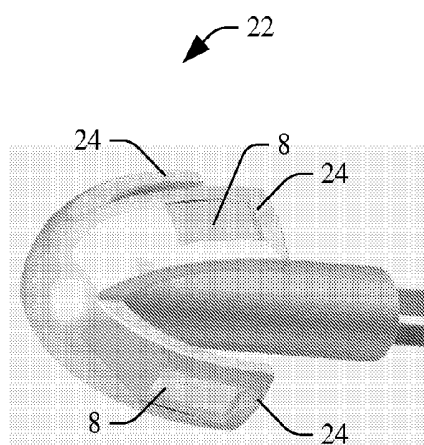


FIGURE 9

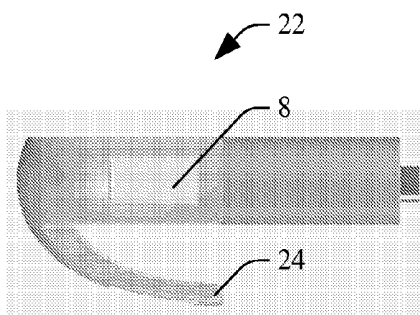


FIGURE 10

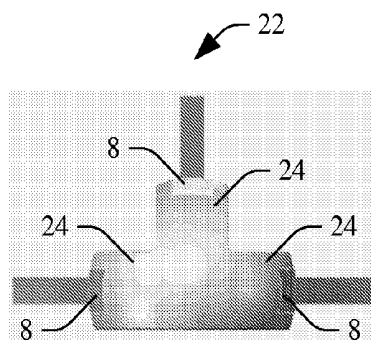


FIGURE 11

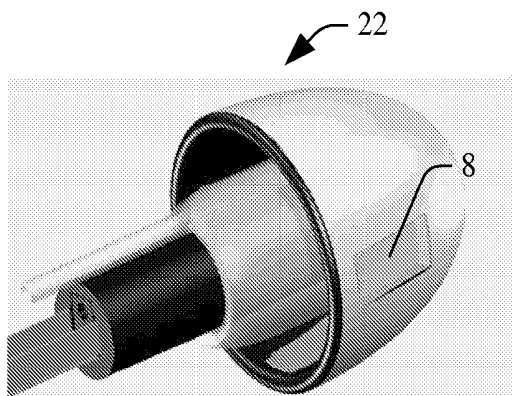


FIGURE 12

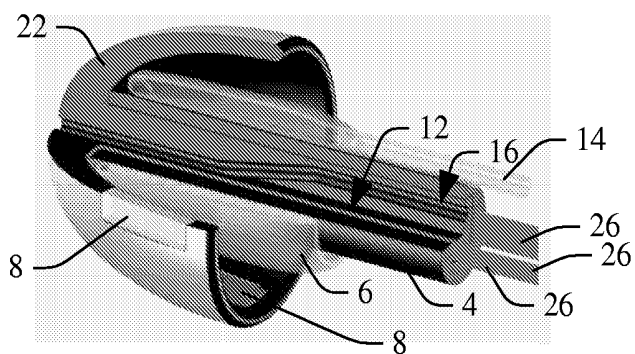


FIGURE 13

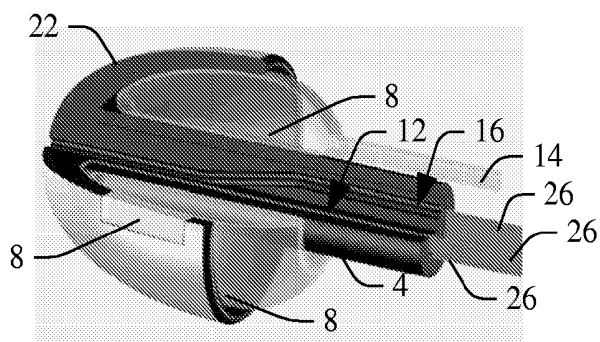


FIGURE 14

# **SIZING AND POSITIONING TECHNOLOGY FOR AN IN-THE-EAR MULTI-MEASUREMENT SENSOR TO ENABLE NIBP CALCULATION**

## **BACKGROUND**

**[0001]** The following relates to monitoring physiology. It finds particular application to an in-the-ear structure that is inserted in the ear canal to suitably position one or more physiological sensors within the inner ear to capture information indicative of physiological phenomena including blood pressure, respiration, perfusion index, blood oxygen, pulse rate, and body temperature, for example.

**[0002]** Physiological signals have been measured from within the ear. However, there are no multi-parameter physiological measurement devices that non-invasively measure blood pressure from within the ear. Examples of barriers that frustrate such development include the varying size and shape of the human ear canal from person to person, an inability to strategically position sensors within the ear canal to optimally receive physiological signals, and an inability to protect sensing devices from contamination through contact with inner ear tissue while measuring physiological signals.

**[0003]** In one aspect, an in-the-ear physiological measurement device includes a structure formed for insertion into an ear canal. One or more sensors are operatively coupled to a portion of the structure that is positioned in the ear. An inflatable balloon is operatively coupled to the portion of the structure positioned in the ear and inflates to position the one or more sensors proximate to tissue within the ear canal. Once suitably positioned, the one or more sensors sense physiological signals from the surrounding tissue and bone structure.

**[0004]** One advantage includes measuring physiological signals from within the ear.

**[0005]** Another advantage resides in non-invasively measuring blood pressure from within the ear.

**[0006]** Another advantage is continuously measuring non-invasive blood pressure from within the ear.

**[0007]** Another advantage resides in an in-the-ear device that forms to different shaped and sized ear canals.

**[0008]** Another advantage is positioning the sensor within the ear canal to optimally receive physiological signals therefrom.

**[0009]** Another advantage is positioning the sensor within the ear canal with ideal force and pressure to ensure close coupling of sensors with tissue without causing blanching of the tissue.

**[0010]** Another advantage is positioning the sensor within a well perfused physiological site even if the body is experiencing peripheral shutdown due to shock or other conditions.

**[0011]** Another advantage is the prevention of over insertion into the ear.

**[0012]** Another advantage is measuring physiological signals through a sheath that mitigates contamination of the physiological sensors.

**[0013]** Another advantage resides in an in-the-ear physiological signal measuring device that equalizes ear pressure with ambient pressure, especially during balloon inflation and deflation.

**[0014]** Still further advantages will become apparent to those of ordinary skill in the art upon reading and understanding the detailed description of the preferred embodiments.

**[0015]** FIG. 1 illustrates an in-the-ear physiological measurement apparatus for measuring physiological signals from within an ear.

**[0016]** FIG. 2 illustrates an in-the-ear physiological measurement apparatus with a single channel for housing sensor wiring and inflating/deflating an inflatable balloon to position sensors proximate to inner ear tissue.

**[0017]** FIG. 3 illustrates an in-the-ear physiological measurement apparatus with separate channels for housing sensor wiring and inflating/deflating an inflatable balloon.

**[0018]** FIG. 4 illustrates an in-the-ear physiological measurement apparatus with an air passage channel for equalizing air pressure between the ear and the environment when inflating and deflating the balloon.

**[0019]** FIG. 5 illustrates an in-the-ear physiological measurement apparatus positioned within an ear.

**[0020]** FIG. 6 illustrates a connection point between an in-the-ear physiological measurement apparatus, a supporting behind-the-ear device, and a protective sheath that mitigates contamination of the physiological sensors.

**[0021]** FIG. 7 illustrates an in-the-ear physiological measurement apparatus connected to a behind-the-ear supporting device.

**[0022]** FIGS. 8-12 illustrate various views of a suitable tip for holding sensors associated with an in-the-ear physiological measurement apparatus.

**[0023]** FIG. 13 is a perspective view in partial section illustrating an uninflated balloon for insertion into the ear canal.

**[0024]** FIG. 14 is a perspective view in partial section illustrating an inflated balloon.

**[0025]** FIG. 1 illustrates an in-the-ear (ITE) physiological measurement apparatus 2 (hereafter "the ITE apparatus 2") for measuring one or more physiological signals (e.g., blood pressure, pulse, blood oxygen, perfusion, temperature, respiration . . . ) from within an ear canal. The ITE apparatus 2 includes a structure 4 that inserts into the ear canal. The structure 4 is dimensioned to enter the ear canal to a suitable depth and adapts to various shaped ear canals (e.g., different curvatures). That is, the structure 4 is small in diameter compared to the diameter of the ear canal. In a preferred embodiment, the structure 4 projects into the ear canal such that an end portion is positioned proximate to a bony region of the ear or other relatively quiet zone of the ear canal.

**[0026]** The end portion of the structure 4 residing in the ear canal includes an annular inflatable balloon 6. The inflatable balloon 6 surrounds the end portion of the structure 4 (as illustrated) or suitable portions thereof. The inflatable balloon 6 ideally supports one or more sensors 8 that are operatively coupled to a surface of the balloon 6 and that measure physiological signals. Suitable sensors include light emitting diodes (LEDs), an infrared (IR) source, light detectors, a pressure transducer, a microphone, and a thermistor, for example. The sensors 8 are strategically positioned on the balloon 6. For example, a light detecting sensor typically is positioned to minimize or prevent absorption of light not indicative of the physiological process under measurement (e.g., light from outside the ear, light emitted from another sensor located on the balloon 6 . . . ). Although depicted as circular in FIG. 1, the one or more sensors 8 can be any shape. Alternatively, the sensors could be mounted within the end portion of the structure 4 and could be moved into contact with the tissue once inserted into the ear.

**[0027]** The inflatable balloon 6 is inflated to position the one or more sensors 8 proximate to appropriate tissue within

the ear canal with ideal force and pressure to ensure close coupling of sensors with tissue but without causing decreased perfusion or blanching of the tissue. For adult humans, this includes inflating the balloon 6 to conform to the widely varying ear canal diameters from about 6 mm to about 13 mm. For neonates and small pediatrics, where the ear canal diameter varies from about 4 mm in diameter to about 7 mm in diameter, smaller and shorter ITE devices are used. Typically, sensors for measuring blood oxygen are positioned proximate to ear canal tissue that is perfused with arterial blood supplied by branches of the External as well as the Internal Carotid Arteries, thus serving as a well perfused physiological site even if the body is experiencing peripheral shutdown due to shock or other conditions. Such sensors include an energy emitting means (e.g., an LED, an IR source . . . ) and an energy detecting means that detects energy transmission through the vascular tissue. In another example, a temperature sensor (e.g., a thermistor) is also positioned proximate to vascular tissue. In yet another example, sensors for sensing audio signals (e.g., a microphone) indicative of pulse pressure sounds, and/or respirations are suitably positioned in relatively quiet regions of the ear canal to mitigate sensing extraneous audio signals (noise).

**[0028]** The inflatable balloon 6 is also used to facilitate non-invasively measuring blood pressure. For a non-invasive blood pressure measurement, the inflatable balloon 6 is inflated until it occludes blood flow in a portion of the ear proximate a blood pressure sensor(s) (e.g., a pressure transducer) operatively connected to the inflatable balloon 6. The pressure in the inflatable balloon 6 is then suitably released to deflate the inflatable balloon 6. A systolic and a diastolic blood pressure are obtained during inflation and/or deflation using an auscultatory approach (e.g., via a microphone operatively connected to the balloon 6) and/or an oscillometric approach (e.g., via optical sensing components attached to the balloon).

**[0029]** A continuous non-invasive blood pressure is measured by obtaining an initial blood pressure measure as describe above and then re-inflating the balloon 6 to a mean pressure. A servo mechanism periodically adjusts balloon pressure to locate a maximum pulse waveform amplitude indicative of mean blood pressure. As long as the derived mean pressure is relatively close to the initial pressure and/or the pulse waveform amplitudes are relatively close, the derived continuous systolic, diastolic, and mean blood pressure are calculated with high accuracy.

**[0030]** The structure 4 includes one or more passageways (as illustrated in FIGS. 2-4 infra) that extend through the structure 4. Such passageways house sensor data, power, and control wires, provide a hermetically sealed channel for inflating/deflating the balloon 6, and/or allow pressure inside the ear to equalize with the environment during balloon inflation/deflation. FIG. 2 depicts an aspect in which the structure 4 includes a channel 10 for both housing sensor wiring and inflating/deflating the balloon 6. The channel 10 isolates the wires from the inner ear environment, mitigating contamination of both the ear and the sensor wiring and provides a pressurized air conduit to the balloon 6. FIG. 3 depicts an aspect in which the structure 4 includes separate channels for sensor wiring and inflating/deflating the balloon 6; one or more first channels 12 house sensor wiring and a second channel 14 provides the pressurized air conduit for inflating/deflating the balloon 6. FIG. 4 depicts an aspect in which an optional channel 16 provides an ear pressure stabilizing

mechanism that allows ear pressure to equalize with the environment during balloon inflation and/or deflation. The channel 16 mitigates pressure build-up in the ear during balloon inflation and/or deflation and potential pain therefrom. The examples in FIG. 2-4 depict the structure 4 and the passageways 10-16 with circular shaped cross-sections. These particular shapes are not limitative and are provided for explanatory purposes. It is to be understood that the structure 4 and/or the passageways 10-16 can be essentially any shape (e.g., oval, rectangular, irregular . . . ) conducive to the ear canal.

**[0031]** FIG. 5 illustrates the ITE apparatus 2 inserted into an ear canal. The structure 4 is inserted such that the end portion with the balloon 6 residing in the ear canal is in a bony region of the ear. The balloon 6 is inflated to position the sensors 8 proximate to inner ear tissue to sense signals indicative of physiological states, including blood pressure, temperature, pulse, respiration, and blood oxygen, for example.

**[0032]** FIG. 6 illustrates the ITE apparatus 2 with an optional sheath 9 placed over the structure 4 and balloon 6 to protect the ear and the structure/balloon/sensor assembly from contamination. In one aspect, the sheath can be semi-permeable to allow air flow, but prevent fluid from moving from one side of the sheath to the other side. In another aspect, the sheath prevents substantially all matter from moving from one side of the sheath to the other side. The structure/balloon/sensor assembly can be disposable, washable, and/or sterilizable.

**[0033]** The structure 4 is shown supported in the ear by a (BTE) ear piece 18. The structure 4 can be operatively attached to the ear piece 18. Such attachment can be through a fastening means including a threaded connector, a snap, a set screw, an adhesive, a rivet, etc. FIG. 6 shows an exemplary connection region 20 between the structure 4 and the optional ear piece 18. A protective sheath 9 may be used to mitigate contamination of the physiological sensors if desired. In another aspect, the structure 4 and the ear piece 18 can be formed as a single unit.

**[0034]** FIG. 7 shows the BTE device 18 connected to the ITE device 2. The ITE device 2 includes a battery 21 which powers both devices. With this embodiment, the ITE device 2 and battery 21 are low cost and disposable.

**[0035]** FIGS. 5-7 above illustrate the optional ear piece 18 as a behind-the-ear supporting device. In a preferred embodiment, the ITE apparatus is connected to a behind-the-ear (BTE) device (18) by means of a semi-rigid connector tube that is formed to fit over and/or around the ear to prevent over insertion and to hold in position the ITE device with optimized orientation and positioning. It is to be understood that other types of supporting devices are contemplated. For example, the structure 4 can be mounted to supporting devices that attach to a region of the head, neck, shoulders, etc.

**[0036]** The BTE device 18 can house various electronics that receive physiological signals from the sensors 8 (e.g., via sensor wire extending through the passageways 10 and 12 briefly described above) and transmit the physiological signals to another transceiver (not shown) worn by the subject (e.g., a transceiver worn around the neck or waist) or to a remote device (not shown) such as a monitoring device, a database, a computer, and a graphical display. The BTE device 18 can optionally include a processor (not shown), memory (not shown), and a battery (not shown). The processor is used to control the sensors and electronics, process raw data, and read data from the sensors; the memory is used to

store data and/or configuration; and the battery powers the processor, active sensors, and the transceiver.

[0037] In the embodiment of FIGS. 8-11, the one or more sensors 8 are located on a soft, pliable tip 22 (rather than directly on the inflatable balloon 6, or on the ITE device tip on a side opposite the inflatable balloon 6) that is operatively connected to the end of the structure 4 inserted into the ear. The balloon 6 is shown in FIG. 8, but has been removed from the FIGS. 9-11 for clarity of illustration. Upon inserting the structure 4 in the ear, the sensors 8 are still positioned by inflating the balloon 6; however, inflating the balloon 6 expands sensor carrying leaves 24 of the tip 22, which positions the sensors 8 proximate to inner ear tissue.

[0038] FIG. 12-14 depict the tip 22 as an expandable mushroom shaped element. In this embodiment, inflating the balloon 6 from the insertion level of FIG. 13 expands the soft, pliable tip 22, which positions the sensors 8 proximate to inner ear tissue (See FIG. 14). The tip 22 and/or balloon 6 also serve as an optical reflector, helping to reflect light from a light emitter through the tissue, from the bone, through the tissue, reflectively and transmissively, to the reflector, from the reflector back through the tissue and so forth, until it finally reaches the light detector. The back side of the tip 22 is opaque which blocks unwanted ambient light coming from within the ear canal. The tip (22) and/or the balloon (6) also serves as buffer between external ambient airflow and thermistor (8) that is measuring a surrogate of core body temperature. Flex-circuit connectors 26 each extend through the structure 4, bend around the balloon 6, and flexibly interconnect with an associated sensor 8.

[0039] The invention has been described with reference to the preferred embodiments. Modifications and alterations may occur to others upon reading and understanding the preceding detailed description. It is intended that the invention be constructed as including all such modifications and alterations insofar as they come within the scope of the appended claims or the equivalents thereof.

1. An in-the-ear (ITE) physiological measurement device, comprising:

- a structure formed for easy insertion into an ear canal;
- one or more sensors operatively coupled to a portion of the structure that is inserted in the ear; and
- an inflatable balloon operatively coupled to the portion of the structure inserted in the ear, the inflatable balloon inflates to position the one or more sensors proximate to tissue within the ear canal such that the one or more sensors can sense physiological signals from the surrounding tissue and bone structure.

2. The ITE physiological measurement device according to claim 1, wherein the one or more sensors non-invasively sense signals indicative of blood pressure, continuous blood pressure, a pulse, a blood oxygen level, perfusion, body temperature, and respiration.

3. The ITE physiological measurement device according to claim 1, wherein the structure is inserted to position the one or more sensors proximate to at least one of a bony region and a quiet zone of the ear canal.

4. The ITE physiological measurement device according to claim 1, wherein the structure is inserted to position the one or more sensors proximate to surrounding deep ear canal tissue which is perfused with arterial blood supplied by branches of at least one of External and Internal Carotid Arteries and

serves as a well perfused physiological site even if the body is experiencing peripheral shutdown due to shock or other conditions.

5. The ITE physiological measurement device according to claim 1, wherein the inflated balloon positions the one or more sensors located thereon proximate to the vascular tissue with ideal force and pressure to ensure close coupling of sensors with tissue without causing decreased perfusion or blanching of the tissue.

6. The ITE physiological measurement device according to claim 1, wherein the one or more sensors are operatively attached to the inflatable balloon.

7. The ITE physiological measurement device according to claim 1, further including a tip operatively connected to a region of the structure inserted in the ear, the one or more sensors being operatively connected to the tip.

8. The ITE physiological measurement device according to claim 7, the tip and/or the balloon serves as a reflector to reflect and direct sensor sourced light through the tissue of the ear, reflectively and transmissively, into a light detector while blocking ambient light.

9. The ITE physiological measurement device according to claim 7, the tip and/or the balloon serves as buffer between external ambient airflow and thermistor that is measuring a surrogate of core body temperature.

10. The ITE physiological measurement device according to claim 7, wherein the balloon is disposed between the structure and the tip to inflate and expand the tip in order to position the one or more sensors located thereon proximate to the vascular tissue.

11. The ITE physiological measurement device according to claim 1, wherein the one or more sensors include one or more of: a light emitting diode, an IR source, a light detector, a thermistor, a pressure transducer, and a microphone.

12. The ITE physiological measurement device according to claim 1, wherein the inflatable balloon expands to position the one or more sensors within an adult ear canal from about 6 mm in diameter to about 13 mm in diameter, and within a pediatric ear canal from about 4 mm in diameter to about 7 mm in diameter.

13. The ITE physiological measurement device according to claim 1, the structure including:

- a passageway that extends through the structure to the balloon for inflating and deflating the balloon.

14. The ITE physiological measurement device according to claim 1, the structure including:

- a passageway that extends through the structure to the one or more sensors for housing sensor wires for carrying power or control signals to the sensors and data from the sensors.

15. The ITE physiological measurement device according to claim 1, the structure including:

- a passageway that extends through the structure (for equalizing ear pressure within the ear canal with ambient air pressure).

16. The ITE physiological measurement device according to claim 1, further including a sheath that protects the structured, the balloon 6, the one or more sensors, and the ear canal from cross contamination.

17. The ITE physiological measurement device according to claim 1, further including a battery that powers one or more components.

18. The ITE physiological measurement device according to claim 1, wherein the ITE physiological measurement



device is operatively connected to the BTE device by means of a semi-rigid connector tube that is formed to fit over and/or around the ear to prevent over insertion and to hold in position the ITE device with optimised orientation and positioning.

**19.** A method for measuring physiological signals within the ear canal, comprising:

inserting an in-the-ear structure into an ear canal to a desired depth;

inflating an inflatable balloon operatively connected to an end portion of the in-the-ear structure to position one or more sensors proximate to vascular tissue of the ear canal; and

using the one or more sensors to sense physiological signals from the surrounding tissue and bone structure.

**20.** The method according to claim **19**, further including measuring blood pressure through the following:

inflating the inflatable balloon to occlude blood flow in the ear tissue proximate to the inflatable balloon; and

obtaining a systolic and a diastolic blood pressure while inflating and/or deflating the inflatable balloon.

**21.** The method according to claim **19**, further including measuring blood pressure through one or more of an auscultatory approach and an oscillometric approach.

**22.** The method according to claim **19**, further including continuously measuring blood pressure through the following:

obtaining at least one of an initial systolic and diastolic blood pressure measure reading;

determining a mean blood pressure measurement from the reading;

inflating the balloon within the ear canal to the mean blood pressure;

periodically adjusting balloon pressure; and

capturing a maximum pulse waveform amplitude indicative of the mean blood pressure.

**23.** The method according to claim **22**, further including deriving at least one of a systolic and a diastolic blood pres-

sure from at least one of the mean blood pressure and one or more pulse waveform amplitudes.

**24.** A physiological measurement device for measuring physiological signals from within the ear canal, comprising:

a first structure formed for easy insertion into multiple shaped and sized ear canals;

a second structure that supports the first structure to facilitate maintaining the position of the first structure within the ear canal;

an inflatable balloon disposed around a portion of the first structure to be positioned in the ear, the inflatable balloon expands radially with inflation;

a radially expanding tip connect with the first structure and extending at least partially around the inflatable balloon such that inflation of the balloon radially expands the tips; and

a sensor carried by the tip to the pressed into sensing interaction within an ear canal.

**25.** The physiological measurement device according to claim **24**, the sensor senses one or more of blood pressure, continuous blood pressure, pulse, blood oxygen level, perfusion, body temperature, and respiration.

**26.** The physiological measurement device according to claim **24**, wherein the one or more sensors include one or more of the following: a light emitting diode, an IR source, a light detector, a thermistor, a pressure transducer, and a microphone.

**27.** The physiological measurement device according to claim **24**, wherein the physiological measurement device is operatively connected to the secondary device by a semi-rigid connector tube that is formed to fit over and/or around the ear to prevent over insertion and to hold the physiological measurement device in position with optimised orientation and positioning.

\* \* \* \* \*

专利名称(译)	用于耳内多测量传感器的尺寸和定位技术，以实现nibp计算		
公开(公告)号	<a href="#">US20090069645A1</a>	公开(公告)日	2009-03-12
申请号	US11/995006	申请日	2006-06-13
[标]申请(专利权)人(译)	皇家飞利浦电子股份有限公司		
申请(专利权)人(译)	皇家飞利浦电子N. V.		
当前申请(专利权)人(译)	皇家飞利浦电子N.V.		
[标]发明人	NIELSEN LARRY POUX CHRISTOPHER J		
发明人	NIELSEN, LARRY POUX, CHRISTOPHER J.		
IPC分类号	A61B5/00		
CPC分类号	A61B5/02 A61B5/021 H04R25/70 A61B5/6817 A61B5/6886 A61B5/14552 A61B5/02116		
优先权	60/695725 2005-06-30 US		
其他公开文献	US8419637		
外部链接	<a href="#">Espacenet</a> <a href="#">USPTO</a>		

#### 摘要(译)

耳内 ( ITE ) 生理测量装置 ( 2 ) 包括形成易于插入多个成形和尺寸的耳道中的结构 ( 4 )。可膨胀气囊 ( 6 ) 围绕结构 ( 4 ) 的端部以定位在耳朵中。可选地，蘑菇形尖端 ( 22 ) 与结构 ( 4 ) 的一端连接并且承载多个传感器 ( 8 )。球囊 ( 6 ) 的膨胀使尖端 ( 22 ) 径向扩张，以将传感器 ( 8 ) 定位在耳道内的血管组织附近。一旦适当定位，一个或多个传感器 ( 8 ) 感测来自血管组织和骨结构的生理信号。

