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(54) **AUTORETROPERFUSION DEVICES AND SYSTEMS**

AUTORETROPERFUSIONSVORRICHTUNGEN UND SYSTEME

DISPOSITIFS DE RÉTROPERFUSION AUTOMATIQUE ET SYSTÈMES

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EP 2 379 130 B1

Description

BACKGROUND

[0001] While direct surgical and percutaneous revascularization through procedures such as a percutaneous transluminal coronary angioplasty ("PTCA") or coronary artery bypass grafting ("CABG") remain the mainstay of treatment for angina and coronary artery disease ("CAD"), there are many cardiac conditions that are not amendable to such conventional revascularization therapies. Because of this, much effort has been made to find alternative methods of revascularization for ischemic cardiac patients who are not candidates for revascularization by conventional techniques. Such patients are generally identified as "no-option" patients because there is no conventional therapeutic option available to treat their condition.

[0002] Currently, there are multiple specific conditions for which conventional revascularization techniques are known to be ineffective as a treatment. Two specific examples of such cardiac conditions include, without limitation, diffuse CAD and refractory angina. Furthermore, a percentage of all patients diagnosed with symptomatic CAD are not suitable for CABG or PTCA. In addition and for various reasons discussed below, diabetic patients - especially those with type 2 diabetes - exhibit an increased risk for having CAD that is not effectively treated by conventional revascularization techniques.

[0003] There is currently little data available on the prevalence and prognosis of patients with symptomatic CAD that is not amendable to revascularization through conventional methods. However, one study indicated that out of five hundred (500) patients with symptomatic CAD who were considering direct myocardial revascularization and angiogenesis, almost twelve percent (12%) were not suitable for CABG or PTCA for various reasons. Furthermore, in general, patients with atherosclerotic involvement of the distal coronary arteries have high mortality and morbidity. For example, a study conducted on patients indicated that, one (1) year after being diagnosed with atherosclerotic involvement of the distal coronary arteries, 39.2% of such patients had had a cardiac-related death, 37.2% had had an acute myocardial infarction, and 5.8% had developed congestive heart failure. Overall, 82.2% of the patients with atherosclerotic involvement of distal coronary arteries had developed or experienced a significant cardiac event within one (1) year.

A. Diffuse CAD and Refractory Angina

[0004] CAD is typically not focal (i.e. limited to one point or a small region of the coronary artery), but rather diffused over a large length of the entire vessel, which is termed "diffuse CAD." Several studies indicate that patients with a diffusely diseased coronary artery for whom standard CABG techniques cannot be successfully performed constitute about 0.8% to about 25.1% of all patients diagnosed with CAD. Furthermore, it is believed that diffuse CAD is much more common than conventionally diagnosed because it is often difficult to detect by an angiogram due to the two-dimensional views.

[0005] Practitioners have realized that the quality of a patient's distal coronary arteries is one of the critical factors related to a successful outcome of a surgical revascularization. As previously indicated, there is considerable evidence that CABG for vessels having diffuse CAD results in a relatively poor outcome. In fact, studies have indicated that diffuse CAD is a strong independent predictor of death after a CABG procedure. Further, as previously noted conventional revascularization techniques have also proven ineffective on a subgroup of patients with medically refractory angina. In line with the aforementioned reasoning, this is likely because patients with medically refractory angina have small or diffusely diseased distal vessels that are not amenable to conventional revascularization therapies. Accordingly, patients exhibiting diffuse CAD or medically refractory angina are often considered no-option patients and not offered bypass surgery, PCTA, or other conventional procedures.

B. Diabetes as a Risk Factor

[0006] Diabetes is an important risk factor for the development of CAD, diffuse or asymptomatic, and it has been estimated that approximately seventy-five percent (75%) of the deaths in diabetic patients are likely attributed to CAD. It is estimated that 16 million Americans have diabetes, without only 10 million being diagnosed. Patients with diabetes develop CAD at an accelerated rate and have a higher incidence of heart failure, myocardial infarction, and cardiac death than non-diabetics.

[0007] According to recent projections, the prevalence of diabetes in the United States is predicted to be about ten percent (10%) of the population by 2025. Further, the increasing prevalence of obesity and sedentary lifestyles throughout developed countries around the world is expected to drive the worldwide number of individuals with diabetes to more than 330 million by the year 2025. As may be expected, the burden of cardiovascular disease and premature mortality that is associated with diabetes will also substantially increase, reflecting in not only an increased amount of individuals with CAD, but an increased number of younger adults and adolescents with type 2 diabetes who are at a two- to four-fold higher risk of experiencing a cardiovascular-related death as compared to non-diabetics.

[0008] In addition to developing CAD at an accelerated rate, CAD in diabetic patients is typically detected in an advanced stage, as opposed to when the disease is premature and symptomatic. Consequently, when diabetic patients are finally diagnosed with CAD they commonly exhibit more extensive coronary atherosclerosis and their epicardial vessels are less amendable to interventional treatment, as compared to the non-diabetic popu-

lation. Moreover, as compared with non-diabetic patients, diabetic patients have lower ejection fractions in general and therefore have an increased chance of suffering from silent myocardial infarctions.

C. No-Option Patients

[0009] Some studies have shown that two-thirds (2/3rds) of the patients who were not offered bypass surgery, because of diffuse CAD or otherwise, either died or had a non-fatal myocardial infarction within twelve (12) months. Furthermore, patients diagnosed with diffuse CAD ran a two-fold increased risk of in-hospital death or major morbidity, and their survival rate at two (2) years was worse than those patients who exhibited non-diffuse CAD or other complicating conditions. As previously indicated, the majority of these patients are considered no-option patients and are frequently denied bypass surgery as it is believed that CABG would result in a poor outcome.

[0010] Due to the increasing numbers of no-option patients and a trend in cardiac surgery towards more aggressive coronary interventions, a growing percentage of patients with diffuse CAD and other no-option indications are being approved for coronary bypass surgery because, in effect, there are no other meaningful treatment or therapeutic options. Some effects of this trend are that the practice of coronary bypass surgery has undergone significant changes due to the aggressive use of coronary stents and the clinical profiles of patients referred for CABG are declining. As such, performing effective and successful coronary bypass surgeries is becoming much more challenging. Bypass grafting diffusely diseased vessels typically requires the use of innovative operations such as on-lay patches, endarterectomies and more than one graft for a single vessel. Patients with "full metal jackets" (or multiple stents) are typically not referred to cardiac surgeons and often end up as no-option patients despite the attempts of using these innovative surgeries.

[0011] In recent decades, the spectrum of patients referred for CABG are older and are afflicted with other morbidities such as hypertension, diabetes mellitus, cerebral and peripheral vascular disease, renal dysfunction, and chronic pulmonary disease. In addition, many patients referred for CABG have advanced diffuse CAD and have previously undergone at least one catheter-based intervention or surgical revascularization procedure that either failed or was not effective. Because of this, the patient's vessels may no longer be graftable and complete revascularization using conventional CABG may not be feasible. An incomplete myocardial revascularization procedure has been shown to adversely affect short-term and long-term outcomes after coronary surgery.

[0012] Due in part to some of the aforementioned reasons, reoperative CABG surgery is now commonplace, accounting for over twenty percent (20%) of cases in some clinics. It is well established that mortality for reoperative CABG operations is significantly higher than primary operations. As such, the risk profile of reoperative patients is significantly increased and such patients are subjected to an increased risk of both in-hospital and long-term adverse outcomes.

[0013] Further, clinicians have also turned to unconventional therapies to treat non-option patients. For example, coronary endarterectomy ("CE") has been used as an adjunct to CABG in a select group of patients with diffuse CAD in order to afford complete revascularization. However, while CE was first described in 1957 as a method of treating CAD without using cardiopulmonary bypass and CABG, this procedure has been associated with high postoperative morbidity and mortality rates and has been afforded much scrutiny. Nevertheless, CE is the only therapeutic option available for many no-option patients with diffuse CAD.

[0014] Similarly, because conventional therapies have proven ineffective or are unavailable to high risk patients, perioperative transmyocardial revascularization ("TMR") has been indicated for patients suffering from medically refractory angina. TMR has proven effective for most patients suffering from refractory angina; the mortality rate after TMR in patients with stable angina ranges between about one to twenty percent (1-20%). Furthermore, in one study, TMR resulted in a higher perioperatively mortality rate in patients with unstable angina than those with stable angina (27% versus 1%). Some even report an operative mortality rate as low as twelve percent (12%). Patients who experience angina and who cannot be weaned from intravenous nitroglycerin and heparin have a significantly higher operative mortality rate (16-27% versus 1-3%). Based on these findings, the clinical practice has been to avoid taking such patients to the operating room for TMR if at all possible. The success of TMR is thought to be due to improved regional blood flow to ischemic myocardium, but the precise mechanisms of its effects remain unclear.

[0015] US5273534 describes a T-tube for evacuating fluids from a bile duct. WO2008/144382A1 describes a device and system for perfusing an oxygenated medium in the cerebral vasculature.

BRIEF SUMMARY

[0016] Disclosed herein are the devices and systems for providing controlling blood perfusion pressure and/or providing retroperfusion to at least one ischemic tissue in a minimally invasive manner. At least some of the disclosed embodiments enable an anastomosis to be formed between a vein and an artery without the use of sutures and through a non-invasive procedure. In addition, various disclosed embodiments provide a cannula device comprising a Y-configuration for bifurcating the arterial flow between an anastomosis and the underlying artery. Examples of the devices, systems and methods described herein can further provide simultaneous au-

toretroperfusion therapy to more than one area of an ischemic tissue.

[0017] In accordance with the present invention, there is provided a catheter for controlling blood perfusion pressure as defined in claim 1.

[0018] In addition, further advantageous embodiments follow from the dependent claims.

[0019] The catheter described herein may further comprise an expandable balloon coupled with the elongated body of the catheter in a position adjacent to where the cannula extends from the elongated body. The expandable balloon may comprise any configuration and, in at least one example, is configured to prevent fluid leakage through an arterial opening when the expandable balloon is in a substantially inflated configuration and the elongated body of the catheter is positioned within an arterial vessel such that the cannula extends through the arterial opening. In this at least one example, the catheter may also comprise a balloon port and a secondary lumen. Here, the balloon port may be in fluid communication with the expandable balloon through a secondary lumen of the catheter. The balloon port may be configured for subcutaneous implantation on a patient or otherwise.

[0020] Systems are also disclosed herein for controlling blood perfusion pressure within a vein. In accordance with the present invention, there is provided a system as defined in claim 8.

[0021] In addition, further advantageous embodiments follow from the dependent claims.

BRIEF DESCRIPTION OF THE DRAWINGS

[0022]

FIG. 1 shows a side view of a catheter for placement within an arterial vessel and that may be used to deliver retroperfusion therapy.

FIG. 2A shows a side view of the catheter of FIG. 1 in a collapsed position.

FIG. 2B shows a side view of the catheter of FIG. 1 in an extended position.

FIG. 3 shows a side view of an autoretroperfusion system positioned to deliver retroperfusion therapy to a heart.

FIGS. 4A and 4B show perspective views of the distal end of a venous catheter used in the autoretroperfusion system of FIG. 3.

FIG. 5 shows the components of an autoretroperfusion system that can be used to deliver retroperfusion therapy to ischemic tissue.

FIG. 6 shows a view of the base and diaphragmatic surface of a heart with the distal ends of two components of the autoretroperfusion system of FIG. 5 positioned therein such that the autoretroperfusion system can deliver simultaneous selective autoretroperfusion therapy thereto.

FIG. 7 shows a flow chart of a method for delivering autoretroperfusion therapy.

FIG. 8A shows a side view of the catheter of FIG. 1 in a collapsed position within an introducer.

FIG. 8B, shows a side view of the catheter of FIG. 1 being introduced via an introducer into an arterial vessel.

FIGS. 8C and 8D show side views of the introducer of FIG. 8A being removed from an arterial vessel, thereby deploying the projection cannula of the catheter of FIG. 1.

FIG. 8E shows a side view of the catheter of FIG. 1 anchored within an arterial vessel through the use of an expandable balloon.

FIG. 9 shows a schematic view of the autoretroperfusion system of FIG. 5 as applied to a heart.

FIG. 10 shows a schematic view of the autoretroperfusion system of FIG. 5 as applied to a heart.

FIG. 11 shows a schematic view of a step of the method of FIG. 7 as the method is applied to a heart.

FIG. 12 shows a flow chart of a method for delivering simultaneously selective autoretroperfusion therapy.

FIG. 13 shows a schematic view of a step of the method of FIG. 12 as the method is applied to a heart.

FIG. 14 shows a schematic view of a step of the method of FIG. 12 as the method is applied to a heart.

DETAILED DESCRIPTION

[0023] It will be appreciated by those of skill in the art that the following detailed description of the disclosed embodiments is merely exemplary in nature and is not intended to limit the scope of the appended claims. The devices, systems, and methods useful for providing selective autoretroperfusion to the venous system and simultaneously achieving the controlled arterialization of the venous systems are discussed in the description. The devices, systems and methods described herein can be used to safely and selectively arterialize venous vessels in order to decrease the stress thereon and prevent rupture of the same. Accordingly, through the use of the devices, systems and methods described herein, long-term autoretroperfusion of oxygenated blood through the coronary venous system can be achieved, thereby providing a continuous supply of oxygen-rich blood to an ischemic area of a tissue or organ. While the devices, systems and methods described herein are described in connection with a heart, it will be understood that such devices, systems and methods are not limited in their application solely to the heart and the same may be used in connection with any ischemic tissue and/or organ in need of an oxygen-rich blood supply.

[0024] Now referring to FIG. 1, a side view of a catheter 10 is shown. The catheter 10 is configured to be placed within an arterial vessel and comprises a flexible, elongated tube having a proximal end 12, a distal end 14 and at least one lumen 15 extending between the proximal end 12 and the distal end 14. The dimensions of the catheter 10 may vary depending on the particulars of a spe-

cific patient or with respect to the artery to be cannulated. For example and without limitation, where the catheter 10 is used to in a system for autoretroperfusion of the coronary sinus, the catheter 10 may comprise a diameter of about 2.7 millimeters to about 4 millimeters (about 8 Fr to about 12 Fr). Furthermore, the at least one lumen 15 of the catheter 10 comprises a sufficient diameter such that blood can flow therethrough. In addition, the catheter 10 may be comprised of any appropriate material, including without limitation, polyurethane or silicone rubber. Furthermore, the catheter 10 may be coated with heparin or any other suitable anti-coagulant such that the catheter 10 may be placed within a vessel for an extended period of time without inhibiting blood flow due to coagulation.

[0025] The distal end 14 of the catheter 10 is configured to allow arterial blood to flow therethrough and into the at least one lumen 15 of the catheter 10. Similarly, the proximal end 12 of the catheter 10 is configured to allow blood within the at least one lumen 15 to flow out of the catheter 10. Accordingly, when the catheter 10 is positioned within an arterial vessel, the oxygenated blood is allowed to flow into the catheter 10 through the distal end 14 of the catheter 10, through the at least one lumen 15, and out of the catheter 10 through the proximal end 12 of the catheter 10. In this manner, placement of the catheter 10 within a vessel does not inhibit the flow of blood through the vessel or significantly affect the pressure of the blood flow within the vessel.

[0026] As shown in FIG. 1, the catheter 10 further comprises a projection cannula 16 that extends from the proximal end 12 of the catheter 10 and forms a Y-shaped configuration therewith. The projection cannula 16 comprises a flexible tube of material that is appropriate for insertion within a vessel and placement within an opening in a vessel wall. Furthermore, the projection cannula 16 comprises at least one lumen 18, a proximal end 20, and a distal end 22. The distal end 22 of the projection cannula 16 is coupled with the body of the catheter 10 and configured to allow the lumen 18 of the projection cannula 16 to communicate with at least one of the at least one lumens 15 of the catheter 10. Accordingly, when blood flows through the at least one lumen of the catheter 10, a portion of the blood flow enters the lumen 18 of the projection cannula 16 through the distal end 22 thereof and flows out through the proximal end 20 of the projection cannula 16. In this manner, the catheter 10 is capable of bifurcating the flow of blood through the vessel in which it is inserted and routing some of that blood flow out of the vessel and to another location.

[0027] This bifurcation can be exploited to modify the pressure of the blood flowing through the projection cannula 16 and/or through the proximal end 12 of the catheter 10 by manipulating the dimensions of the projection cannula 16 and the body of the catheter 10. For example, and without limitation, if the diameter of the projection cannula 16 is less than the diameter of the at least one lumen 15 of the catheter 10, the majority of the blood will flow through the proximal end 12 of the catheter 10 and the pressure of the remaining blood that flows through the smaller projection cannula 16 will necessarily be reduced. Predictably, the smaller the diameter of the lumen 18 of the projection cannula 16, the greater the pressure drop that can be achieved in the blood flowing through the lumen 18 of the projection cannula 16. Accordingly, with respect to the catheter's 10 application to autoretroperfusion therapies, the projection cannula 16 can be used to re-route blood flow from an artery to a vein while simultaneously achieving the necessary pressure drop in the re-routed blood between the arterial system and unarterialized venous system. Moreover, the catheter 10 is capable of maintaining substantially normal blood flow through the artery in which it is housed as the arterial blood not re-routed through the projection cannula 16 is allowed to flow through the open proximal end 12 of the catheter 10 and back into the artery in the normal antegrade fashion.

[0028] Due to the configuration of the projection cannula 16 and the material of which it is comprised, the projection cannula 16 is capable of hingedly moving relative to the body of the catheter 10 between a collapsed position and an extended position. Now referring to FIGS. 2A and 2B, the projection cannula 16 is shown in the collapsed position (FIG. 2A) and in the extended position (FIG. 2B). When the projection cannula 16 is in the collapsed position, the projection cannula 16 is positioned substantially parallel with the body of the catheter 10. Alternatively, when the projection cannula 16 is in the extended position, the projection cannula 16 is positioned such that the projection cannula 16 forms an angle θ with the proximal end 12 of the catheter 10. The value of angle θ may be selected depending on the desired application of the catheter 10. The angle θ may comprise any value ranging between about 15° and about 90°. In one example, the angle θ may comprise about 45° when the projection cannula 16 is in the extended position.

[0029] The projection cannula 16 is biased such that, when it is not subject to a downward force, the projection cannula 16 rests in the expanded position. Conversely, when a downward force is applied to the projection cannula 16 by way of an introducer or otherwise, the projection cannula 16 moves into and remains in the collapsed position until the downward force is removed. In this manner, the projection cannula 16 may be introduced into a vessel in the collapsed position through the use of an introducer or shaft and thereafter move into the expanded position when the catheter 10 is properly positioned within the vessel and the introducer or shaft is removed.

[0030] Optionally, as shown in FIG. 1, the catheter 10 may further comprise an expandable balloon 58 coupled with an intermediary portion of the external surface of the catheter 10 such that the expandable balloon 58 encases the catheter 10 and the distal end 22 of the projection cannula 18. The expandable balloon 58 may be any expandable balloon 58 that is appropriate for insertion within a vessel and may comprise any material suitable for this function, including without limitation, polyethylene,

latex, polyestherurethane, polyurethane, sylastic, silicone rubber, or combinations thereof. In operation, the expandable balloon 58 can be used to anchor the catheter 10 in a desired position within a vessel wall and prevent leakage from the opening in the vessel wall through which the projection cannula 16 traverses.

[0031] The expandable balloon 58 is capable of being controlled by a clinician such that it can inflate and/or deflate to the proper size. The sizing of the expandable balloon 58 will differ between patients and applications. The expandable balloon 58 may be in fluid communication with a balloon inflation port 62 through a secondary lumen 60 within the lumen 18 of the projection cannula 16. Alternatively, the expandable balloon 58 may be in fluid communication with the balloon inflation port 62 through a tube or other means that is positioned within the lumen 18 of the projection cannula 16 as shown in FIG. 1. The balloon port 62 may be positioned subcutaneously or otherwise such that a clinician can easily access the balloon port 62 when the catheter 10 is positioned within a vessel. In this manner the balloon port 62 can be accessed by a clinician, subcutaneously, percutaneously or otherwise, and used to inflate or deflate the expandable balloon 58 with no or minimal invasion to the patient.

[0032] Now referring to FIG. 3, an autoretroperfusion system 100 is shown positioned to allow arterial blood to irrigate the coronary sinus of a heart 101. With respect to the heart 101, the autoretroperfusion system 100 may be used for treatment of myocardial infarctions by injecting arterial blood into the coronary sinus in synchronism with the patient's heartbeat. Furthermore, the autoretroperfusion system 100 is capable of controlling the pressure of the arterial blood flow as it enters the venous vessel such that when the arterial blood flow is first introduced into the venous system, the pressure of the re-routed arterial blood flow is reduced to protect the thinner venous vessels. In this manner, the venous system is allowed to gradually arterialize. Further, after the selected venous vessel has sufficiently arterialized, the autoretroperfusion system 100 is capable of reducing or ceasing its influence on the pressure of the re-routed arterial blood flow such that the standard arterial blood flow pressure is thereafter allowed to flow into the arterialized venous vessel.

[0033] Autoretroperfusion system 100 comprises the catheter 10, a second catheter 150, and a connector 170. The catheter 10 is for placement within an arterial vessel and is configured as previously described in connection with FIGS. 1-2B. The second catheter 150 is configured for placement within the venous system. The connector 170 is configured to form an anastomosis between the catheter 10 and the second catheter 150 and further functions to monitor various data points on the blood flow flowing therethrough. In addition, in at least one example, the connector 170 is capable of controlling the pressure of arterial blood flowing therethrough.

[0034] The second catheter 150 is configured for placement within a venous vessel wall 114 and comprises a flexible tube having a proximal end 152, a distal end 154 and at least one lumen 156 extending between the proximal end 152 and the distal end 154. Both the proximal end 152 and the distal end 154 of the second catheter 150 are open and in communication with the at least one lumen 156 of the second catheter 150, thereby allowing blood to flow into the at least one lumen 156 through the proximal end 152 and out of the distal end 154 back into the venous vessel 114. The second catheter 150 may be any catheter known in the art that is capable of intravascular insertion and advancement through the venous system and may comprise any appropriate material, including without limitation, polyurethane or silicone rubber. In at least one example, the second catheter 150 is configured to receive a guidewire 510 (see FIGS. 4A and 4B) through the at least one lumen 156 to facilitate the intravascular delivery of the distal end 154 of the second catheter 150 into the desired location of the venous vessel 114. Furthermore, similar to the catheter 10, the second catheter 150 may be coated with heparin or any other suitable anti-coagulant prior to insertion in order to facilitate the extended placement of the second catheter 150 within the venous vessel 114. Accordingly, the autoretroperfusion system 100 may be used to deliver chronic retroperfusion treatment to an ischemic area of a body.

[0035] FIGS. 4A and 4B show side views of the distal end 154 of the second catheter 150 positioned within the venous vessel wall 114. As shown in FIG. 4A, the distal end 154 of the second catheter 150 may further comprise an expandable balloon 158 coupled with the external surface of the second catheter 150. In operation, the expandable balloon 158 can be used to anchor the distal end 154 of the second catheter 150 in the desired location within the venous vessel wall 114. The expandable balloon 158 may be any expandable balloon that is appropriate for insertion within a vessel and can be formed of any material suitable for this function, including without limitation, polyethylene, latex, polyestherurethane, polyurethane, sylastic, silicone rubber, or combinations thereof.

[0036] The expandable balloon 158 is capable of being controlled by a clinician such that it can inflate and/or deflate to the proper size. The sizing of the expandable balloon 158 will differ between patients and applications and it is often important to determine the proper sizing of the expandable balloon 158 to ensure the distal end 154 of the second catheter 150 is securely anchored within the desired location of the vessel wall 114. The accurate size of the expandable balloon 158 can be determined through any technique known in the art, including without limitation, by measuring the compliance of the expandable balloon 158 *ex vivo* or *in vivo.* In addition, the distal end 154 of the second catheter 150 may further comprise a plurality of electrodes that are capable of accurately measuring the cross-sectional area of the vessel of interest as is known in the art. For example, the plurality

of electrodes may comprise a combination of excitation and detection electrodes as described in detail in the currently pending U.S. Patent Application No. 11/891,981 entitled System and Method for Measuring Cross-Sectional Areas and Pressure Gradients in Luminal Organs, and filed on August 14, 2007. In at least one embodiment, such electrodes may comprise impedence and conductance electrodes and may be used in connection with ports for the suction of fluid from the vessel and/or the infusion of fluid therein.

[0037] The expandable balloon 158 may be in fluid communication with a secondary lumen 160 disposed within the at least one lumen 156 of the second catheter 150. In this example, the secondary lumen 160 is coupled with a balloon port 162 that extends from the proximal end 152 of the second catheter 150 (see FIG. 3). Accordingly, when the autoretroperfusion system 100 is positioned within a patient, the balloon port 162 can be easily accessed by a clinician, subcutaneously, percutaneously or otherwise, and used to inflate or deflate the expandable balloon 158 with no or minimal invasion to the patient.

[0038] As shown in FIGS. 4A and 4B, the distal end 154 of the second catheter 150 may further comprise at least one sensor 166 coupled therewith. In at least one example, the at least one sensor 166 is disposed on the distal end 154 of the second catheter 150 distally of the expandable balloon 158; however, it will be understood that the at least one sensor 166 may be disposed in any location on the distal end 154 of the second catheter 150.

[0039] The at least one sensor 166 may be used for monitoring purposes and, for example, may be capable of periodically or continuously monitoring the pressure of the blood flow flowing through the at least one lumen 156 of the first catheter 150 or the venous vessel 14 in which the second catheter 150 is inserted. Additionally, one of the at least one sensors 166 may be used to monitor the pH or the concentrations of carbon dioxide, lactate, or cardiac enzymes within the blood. Furthermore, the at least one sensor 166 is capable of wirelessly communicating the information it has gathered to a remote module through the use of telemetry technology, the internet, or other wireless means, such that the information can be easily accessed by a clinician on a real-time basis or otherwise.

[0040] Now referring back to FIG. 3, the autoretroperfusion system 100 further comprises a connector 170. The connector 170 comprises any connector or quick connector known in the medical arts that is capable of forming an anastomosis between an artery and a vein such that oxygenated blood from the arterial system can flow into the venous system. For example, the connector 170 may comprise an annular connector that is capable of coupling with the proximal end 20 of the projection cannula 16 of the catheter 10 and with the proximal end 152 of the second catheter 150 such that arterial blood can flow continuously from the at least one lumen 15 of the catheter 10 to the at least one lumen 156 of the second catheter 150. The connector 170 may be formed of any suitable material known in the art including, but not limited to, silicon rubber, poly(tetrafluoroethene), and/or polyurethane.

[0041] The connector 170 of the autoretroperfusion system 100 may comprise a pressure/flow regulator unit that is capable of measuring the flow rate of the blood moving therethrough, the pressure of the blood moving therethrough, and/or other data regarding the blood flowing through the anastomosis. The connector 170 may also be capable of transmitting such gathered data to a remote module 180 through a lead placed intravascularly or, in the alternative, through telemetry or another wireless means. The remote module 180 may comprise any device capable of receiving the data collected by the connector 170 and displaying the same. For example, and without limitation, the remote module 180 may comprise any display device known in the art or a computer, a microprocessor, hand-held computing device or other processing means.

[0042] Additionally, the connector 170 may further comprise a means for regulating the blood flow through the anastomosis. One of the main challenges of successfully delivering retroperfusion therapies is that the arterial blood pressure must be reduced prior to being introduced into a vein due to the thinner and more fragile anatomy of venous walls. Indeed, subjecting a non-arterialized venous vessel to the high pressures of arterial blood flow typically results in rupture of the venous vessel. Accordingly, with retroperfusion therapies, it is critical to ensure that the pressure of the arterial blood flow is at least initially controlled such that the venous vessel can arterialize prior to being subjected to the unregulated pressure of the arterial blood flow.

[0043] In at least one example the connector 170 may comprise an external compression device to facilitate the control of the flow rate of the blood moving through the anastomosis. Alternatively, other means that are known in the art may be employed to regulate the blood flow and pressure of the blood flowing through the anastomosis formed by the connector 170. In at least one example, the means for regulating the blood flow through the anastomosis formed by the connector 170 is capable of regulating the pressure and/or flow velocity of the blood flowing through the anastomosis. For example, the means for regulating blood flow can be adjusted to ensure that about a 50 mg Hg pressure drop occurs in the blood flow between the arterial vessel and the venous vessel.

[0044] The connector 170 is capable of not only transmitting data to the remote module 180, but also receiving commands from the remote module 180 and adjusting the means for regulating blood flow pursuant to such commands. Accordingly, when the autoretroperfusion system 100 is positioned within a patient for retroperfusion therapy, a clinician can use the remote module 180 to view the blood flow data collected by the connector 170 and non-invasively adjust the connector 170 to achieve the desired pressure and/or flow through the

anastomosis. Such remote control of the connector 170 is particularly useful as a clinician may incrementally decrease the connector's 170 regulation of the blood flow without surgical intervention during the venous arterialization process and/or after the venous vessel arterializes.

[0045] Further, where the remote module 180 comprises a computer or other processing means, the remote module 180 is also capable of being programmed to automatically analyze the data received from the connector 170 and, based on the results thereof, suggest how to adjust the means of regulating the blood flow of the connector 170 and/or automatically adjust the means of regulating the blood flow of the connector 170 to achieve the optimal result. For example, and without limitation, when the autoretroperfusion system 100 is implanted into a patient and the anastomosis is first performed, the remote module 180 can automatically adjust the means for regulating the blood flow of the connector 170 based on the initial blood flow data received by the remote module 180. In this manner, the desired pressure drop between the arterial system and the venous system is immediately achieved and the risk of venous rupture is significantly reduced.

[0046] Alternatively, where the connector 170 of the autoretroperfusion system 100 does not comprise a means for regulating blood flow, the gradual arterialization of the venous vessel can be achieved through other techniques known in the art. For example, in at least one arrangement, the autoretroperfusion system 100 further comprises a coil designed to at least partially occlude the vein of interest. In this manner, the pressure is allowed to build in front of the portion of the vein at least partially occluded by the coil and the vein gradually arterializes. In this at least one arrangement, the coil may comprise a metallic memory coil (made of nitinol, stainless steel or other acceptable materials that are radioopaque) and is covered with polytetrafluorethylene, polyethylene terephthalate, polyurethane or any other protective covering available in the medical arts.

[0047] Additionally, gradual arterialization can be performed by the second catheter 150. In this example of autoretroperfusion system 100, the at least one lumen 156 of the second catheter 150 is designed to provide an optimal stenosis geometry to facilitate the desired pressure drop as the arterial blood flows therethrough and into the venous system. For example, and without limitation, the at least one lumen 156 may further comprise an internal balloon or resorbable stenosis as disclosed in International Patent Application No. PCT/US2006/029223, entitled "Devices and Methods for Controlling Blood Perfusion Pressure Using a Retrograde Cannula," filed July 28, 2006,.

[0048] In at least one example, the stenosis comprises an internal expandable balloon (not shown) positioned within the lumen 156 of the second catheter 150. In this at least one example, the internal expandable balloon can be used to provide a pressure drop between the arterial and venous systems as is required to achieve the gradual arterialization of the target vein. The internal expandable balloon and the external expandable balloon 158 of the second catheter 150 may positioned concentrically or, alternatively, the internal expandable balloon and the expandable balloon 158 may be coupled with distinct portions of the second catheter 150.

[0049] The internal expandable balloon may comprise any material suitable in the medical arts, including, without limitation, polyethylene, latex, polyestherurethane, polyurethane, sylastic, silicone rubber, or combinations thereof. Further, the internal expandable balloon may be in fluid communication with a tertiary lumen (not shown) disposed within the at least one lumen 156 of the second catheter 150. In this example, the tertiary lumen is also in fluid communication with an internal balloon port that extends from the proximal end 152 of the second catheter 150. Accordingly, the internal balloon port can be easily accessed by a clinician, subcutaneously, percutaneously or otherwise, and the internal balloon port can be used to inflate or deflate the internal expandable balloon with minimal or no discomfort to the patient when the system 100 is in operation. Alternatively, the internal expandable balloon may be in fluid communication with the at least one lumen 156 of the second catheter 150. In this example, the arterial blood flow through the at least one lumen 156 functions to inflate and deflate the internal expandable balloon in conjunction with the systolic and diastolic components of a heart beat.

[0050] The internal expandable balloon may be sized to a specific configuration in order to achieve the desired stenosis. In one example, the size of the desired stenosis may be obtained by measuring the pressure at the tip of the distal end 156 of the second catheter 150 with the at least one sensor 166 while the internal expandable balloon is being inflated. Once the desired intermediate pressure is obtained, the internal expandable balloon volume may then be finalized and the vein is thereafter allowed to arterialize at the modified pressure for a defined period of time. At the end of the defined period (typically about 2-3 weeks), the internal expandable balloon may be removed from the at least one lumen 156 of the second catheter 150.

[0051] Insertion and/or removal of the internal expandable balloon from the system 100 may be achieved through the internal balloon port and the related tertiary lumen of the second catheter 150. For example, if the internal expandable balloon is no longer necessary to control the pressure on the venous system because the arterialization of the vein is substantially complete, the internal expandable balloon can be deflated through use of internal balloon port and withdrawn from the system 100 through the tertiary lumen and the internal balloon port.

[0052] Other examples of the system 100 may comprise other suitable means for providing a stenosis within the at least one lumen 156 of the second catheter 150 such that a pressure drop is achieved in blood flowing

therethrough. For example, while a stenosis can be imposed by inflation of the internal expandable balloon, it may also be imposed through positioning a resorbable material within the at least one lumen 156 of the second catheter 150. The resorbable stenosis may be comprised of a variety of materials including, for example and without limitation, magnesium alloy and polyols such as mannitol, sorbitol and maltitol. The degradation rate of the resulting resorbable stenosis will be dependent, at least in part, upon on what type of material(s) is selected to make-up the resorbable stenosis and the same may be manipulated to achieve the desired effect.

[0053] In addition to the aforementioned components of the autoretroperfusion system 100, the autoretroperfusion system 100 may further include a first graft 185 and a second graft 190 as shown in FIG. 3. In this example, the first graft 185 is coupled with the proximal end 20 of the projection cannula 16 (that extends through the exterior arterial wall 116) and the connector 170. Further, the second graft 190 is coupled with the proximal end 152 of the second catheter 150 (positioned within the venous vessel wall 114) and the connector 170. Accordingly, in this at least one example, the second graft 190 is capable of traversing the venous vessel wall 114 in such a manner that the anastomosis is sealed and no blood flow is allowed to leak from the anastomosed vein 114.

[0054] In this manner, the first and second grafts 185, 190 facilitate the formation of an elongated anastomosis between the venous and arterial vessels 114, 116 and thereby relieve any pressure that may be applied to the two vessels 114, 116 due to the anastomosis formed therebetween. For example and without limitation, in at least one example the combined length of the grafts 185, 190 and the connector 170 is about 6 centimeters. However, it will be understood that the grafts 185, 190 may comprise any length(s) so long as the dimensions allow for an anastomosis to form between the applicable vessels and a fully developed blood flow is achieved from the artery to the venous vessel of interest.

[0055] Alternatively, the autoretroperfusion system 100 may only comprise the second graft 190 in addition to the catheter 10, the second catheter 150 and the connector 170. In this example, the connector 170 is coupled with the proximal end 20 of the projection cannula 16 and the second graft 190. Furthermore, the second graft 190 is further coupled with the proximal end 152 of the second catheter 150 such that the second graft 190 traverses an opening within the venous vessel wall 114 (see FIG. 5).

[0056] The grafts 185, 190 may comprise any biocompatible, non-resorbable material having the necessary strength to support the surrounding tissue and withstand the pressure asserted by the blood flow therethrough. Furthermore, the grafts 185, 190 must exhibit the necessary flexibility to form an anastomosis between the vein and the artery within which the catheter 10 and the second catheter 150 are respectively housed. For example, and without limitation, the grafts 185, 190 may comprise any conventional implant including synthetic and natural prosthesis, grafts, and the like. The grafts 185, 190 may also comprise a variety of suitable materials, including those conventionally used in anastomosis procedures, including, without limitation, natural and synthetic materials such as heterologous tissue, homologous tissue, polymeric materials, Dacron, fluoropolymers, and polyurethanes. For example, and without limitation, the first and second grafts 185, 190 may comprise a material such as GORE-TEX (polytetraflouroethylene). The grafts 185, 190 may be coated with heparin or any other suitable anti-coagulant. Accordingly, the first graft 185 and the second graft 190 may be placed within a vessel or have blood flow therethrough for an extended period of time without inhibiting blood flow due to coagulation.

[0057] In at least one example of the autoretroperfusion system 100, the components of the system 100 are available in a package. Here, the package may also contain at least one sterile syringe containing the fluid to be injected into the balloon port 62 to inflate the expandable balloon 58 of the catheter 10 and/or the balloon port 162 to inflate the expandable balloon 158 of the second catheter 150. Furthermore, the package may also contain devices to facilitate delivery of the autoretroperfusion system 100 such as venous and arterial access devices, a expandable balloon 58 of the catheter 10 and/or the balloon port 162 to inflate the expandable balloon 158 of the second catheter 150. Furthermore, the package may also contain devices to facilitate delivery of the autoretroperfusion system 100 such as venous and arterial access devices, a delivery catheter, a guidewire and/or mandrel, an introducer to maintain the catheter 10 in the collapsed position during delivery and, in those examples where a coil is used to arterialize the vein of interest, a pusher bar as is known in the art.

[0058] The guidewire used to facilitate the delivery of the autoretroperfusion system 100 into a vessel by providing support to the components thereof. The guidewire may comprise any guidewire known in the art. Furthermore, the distal end of the guidewire may comprise a plurality of impedance electrodes that are capable of taking measurements of the size the vessel in which the guidewire is inserted through the use of impedance technology. Additionally, in at least one example, the impedance electrodes may be further capable of communicating such measurements to the remote module 180 through telemetry or other wireless means in a manner similar to the at least one sensor 166 of the distal end 154 of the second catheter 150. In at least one example, the distal end of the guidewire may comprise two tetrapolar sets of impedance electrodes disposed on its distalmost tip.

[0059] Based on the information gathered by the impedance electrodes, a clinician can obtain accurate measurements of a selective region of a vessel. In this manner, the expandable balloon 158 coupled with the distal end 154 of the second catheter 150 may be properly sized and the amount of fluid or gas needed to inflate the

expandable balloon 158 can be determined prior to introducing the second catheter 150 into the vein of interest. For example, a clinician can use the plurality of impedance electrodes on the guidewire to obtain measurements of the size and shape of the sub-branches of the coronary sinus. Details regarding the specifications and use of the impedance electrodes are described in detail in the currently pending United States Patent Application No. 10/782,149 entitled "System and Method for Measuring Cross-Sectional Areas and Pressure Gradients in Luminal Organs," and filed on February 19, 2004.

[0060] Now referring to FIG. 5, components of a simultaneous selective autoretroperfusion system 300 are shown. The simultaneous selective autoretroperfusion system 300 (the "SSA system 300") are configured identically to the autoretroperfusion system 100 except that the SSA system 300 further comprises a third catheter 350 and a Y connector 320, both configured for placement within the venous vessel wall 114. Specifically, the SSA system 300 comprises the catheter 10, the second catheter 150, the third catheter 350, the connector

[0061] The third catheter 350 is configured for placement within the venous vessel wall 114 adjacent to the second catheter 150. The third catheter 350 is configured identically to the second catheter 150 and comprises a flexible tube having a proximal end 352, a distal end 354 and at least one lumen 356 extending between the proximal end 352 and the distal end 354. Both the proximal end 352 and the distal end 354 of the third catheter 350 are open and in communication with the at least one lumen 356 of the third catheter 350, thereby allowing blood to flow into the at least one lumen 356 through the proximal end 352 and out of the distal end 354 back into the venous vessel 114.

[0062] The third catheter 350 may be any catheter known in the art that is capable of intravascular insertion and advancement through the venous system. The third catheter 350 may comprise any appropriate material, including without limitation, polyurethane or silicone rubber. In at least one example, the third catheter 350 is configured to receive a guidewire 310 (see FIGS. 5 and 6) through the at least one lumen 356 in order to facilitate the intravascular delivery of the distal end 354 of the third catheter 350 into the desired location of the venous vessel 114. Furthermore, the third catheter 350 is coated with heparin or any other suitable anti-coagulant prior to insertion in order to facilitate the extended placement of the third catheter 350 within the venous vessel 114.

[0063] As shown in FIG. 5, the distal end 354 of the third catheter 350 further comprises an expandable balloon 358 coupled with the external surface of the third catheter 350. In operation, the expandable balloon 358 can be used to anchor the distal end 354 of the third catheter 350 in the desired location within the venous vessel wall 114. The expandable balloon 358 may be any expandable balloon that is appropriate for insertion within a vessel and can be formed of any material suitable for this function, including without limitation, polyethylene, latex, polyestherurethane, polyurethane, sylastic, silicone rubber, or combinations thereof.

[0064] Similar to the expandable balloon 158 of the second catheter 150, the expandable balloon 358 is capable of being controlled by a clinician such that it can inflate and/or deflate to the proper size. The appropriate size of the expandable balloon 358 can be determined through any technique known in the art, including without limitation, by measuring the compliance of the expandable balloon 358 *ex vivo or in vivo.* Furthermore, when the guidewire 310 is used to facilitate the delivery of the distal end 354 of the third catheter 350 into the desired location within the venous vessel wall 114, the electrodes on the distal end of the guidewire 310 may be used to accurately measure the cross-sectional area of the venous vessel 114 such that the expandable balloon 358 can be precisely sized prior to insertion into the vein 114.

[0065] In this at least one example, the expandable balloon 358 is in fluid communication with a secondary lumen 360 disposed within the at least one lumen 356 of the third catheter 350. In this example, the secondary lumen 360 is coupled with a balloon port 362 that extends from the proximal end 352 of the third catheter 350. Accordingly, when the SSA system 300 is positioned within a patient, the balloon port 362 can be easily accessed by a clinician, subcutaneously, percutaneously or otherwise, and used to inflate or deflate the expandable balloon 358 with no or minimal invasion to the patient.

[0066] Similar to the second catheter 150, the distal end 354 of the third catheter 350 may further comprise at least one sensor 366 coupled therewith. The at least one sensor 366 may be configured identically to the at least one sensor 166 of the second catheter 150 and, accordingly, the at least one sensor 366 may be used to monitor the pressure of blood flow through the at least one lumen 356 of the third catheter 350 or the venous vessel 114 or to monitor the pH or the concentrations of carbon dioxide, lactate, or cardiac enzymes within the blood. Furthermore, the at least one sensor 366 is capable of communicating the data it gathers to the remote module 180 through the use of a wireless technology such that a clinician can easily access the gathered information on a real-time basis or otherwise. In at least one example, the at least one sensor 366 is disposed on the distal end 354 of the third catheter 350 distally of the expandable balloon 358; however, it will be understood that the at least one sensor 366 may be disposed in any location on the distal end 354 of the third catheter 350.

[0067] The Y connector 320 of the SSA system 300 comprises flexible material and has a proximal end 322, a distal end 324 and at least one lumen 326 extending between the proximal and distal ends 322, 324. The proximal end 322 of the Y connector 322 is open and configured to be securely coupled with the graft 190. The distal end 324 of the Y connector 322 comprises two open ends which extend from the body of the Y connector 322 in a substantially Y-shaped configuration. The two open ends of the distal end 324 of the Y connector 322 thereby divide

the at least one lumen 326 into two separate channels and thus the blood flowing through the at least one lumen 326 is yet again bifurcated.

[0068] The proximal end 152 of the second catheter 150 is coupled with one of the two open ends of the distal end 324 of the Y connector 322, thereby receiving a portion of the blood flow that flows through the at least one lumen 326 of the Y-connector. Similarly, the proximal end 352 of the third catheter 350 is coupled with the other open end of the distal end 324 of the Y connector 322 and, thus, the third catheter receives a portion of the blood flow that flows through the at least one lumen 326 of the Y-connector. In this manner, the SSA system 300 can be used to simultaneously retroperfuse more than one ischemic area of the body.

[0069] In application, the second catheter 150 and the third catheter 350 are positioned adjacent to each other within the venous vessel wall 114 as shown in FIG. 5. Furthermore, the distal ends 154, 354 of the second and third catheters 150, 350, respectively, may be placed within different veins such that the arterial blood is delivered to selective portions of ischemic tissue. For example, as shown in FIG. 6, in at least one example the SSA system 300 can be applied to a heart 314 to provide an arterial blood supply to two separate coronary veins, or sub-branches, simultaneously. In this at least one example, the distal ends 154, 354 of the second and third catheters 150, 350 are both advanced through the coronary sinus 370. As the diameter of the coronary sinus 370 ranges from about 10 to about 20 millimeters, cannulating the coronary sinus 370 with both the second and third catheters 150, 350 does not occlude the normal antegrade flow of the blood therethrough. Upon reaching the veins or sub-branches of interest, the distal ends 154, 354 of the second and third catheters 150, 350 are each independently positioned within the veins of interest. In the example shown in FIG. 6, the second catheter 150 is positioned within the interventricular vein 374 and the distal end 354 of the third catheter 350 is positioned within the middle cardiac vein 376. As with autoretroperfusion system 100, the expandable balloons 158, 358 are inflated through balloon ports 162, 362, respectively (shown in FIG. 5), such that the distal ends 154, 354 of the second and third catheters 150, 350 are securely anchored in the desired location within the veins of interest. In this manner, the SSA system 300 can deliver controlled arterial blood flow to, and thus arterialize, two areas of the heart 314 simultaneously.

[0070] In at least one example of the SSA system 300, the components of the system 300 are available in a package. Here, the package may also contain sterile syringes with the fluids to be injected into the balloon ports 162, 362 to inflate the expandable balloons 158, 358, respectively. Furthermore, the package may also contain devices to facilitate delivery of the SSA system 300 such as arterial and venous access devices, a delivery catheter, at least two guidewires (configured as described in connection with the delivery of autoretroperfusion system 100), an introducer to maintain the catheter 10 in the collapsed position during delivery and, in those examples where a coil is used to arterialize the vein of interest, a pusher bar as is known in the art.

[0071] Now referring to FIG. 7, a flow chart of a method 400 for performing automatic retroperfusion using the system 100 is shown. While the method 400 is described herein in connection with treating a heart through catheterization of the coronary sinus, it will be understood that the method 400 may be used to perform autoretroperfusion on any organ or tissue in need of retroperfusion treatment.

[0072] Method 400, and the examples thereof, can be performed under local anesthesia and do not require any arterial sutures. Further, once implanted, the system 100 can deliver chronic treatment to the patient as the system 100 is capable of remaining within a patient's vascular system for an extended period of time. In this manner, the system 100 and method 400 can be used to treat no-option patients and greatly enhance their quality of life.

[0073] As shown in FIG. 7, in one approach to the method 400, at step 402 an artery 502 of interest is percutaneously punctured under local anesthesia with a conventional artery access device or as otherwise known in the art. For example and without limitation, in at least one example, an 18 gauge needle is inserted into the femoral or subclavian artery. At step 404, the catheter 10 housed in a collapsed position within an introducer 504 (see FIG. 8A) is inserted into the artery 502 of interest. After the distal end 14 of the catheter 10 is positioned in the desired location within the artery 502, the introducer 504 is proximally withdrawn from the artery 502 as shown in FIG. 8B, leaving the catheter 10 positioned therein.

[0074] In at least one example, the projection cannula 16 is configured such that when the introducer 504 is withdrawn in a proximal direction, the proximal end 12 of the catheter 10 is released from the introducer 504 before the proximal end 20 of the projection cannula 16 is released from the introducer 504. In this manner, the proximal end 12 of the catheter 10 is delivered within the interior of the arterial wall 502, while the projection cannula 16 remains housed within the interior of the introducer 504 as shown in FIG. 8C. Furthermore, because the introducer 504 no longer applies downward pressure to the projection cannula 16 relative to the proximal end 12 of the catheter 10, the projection cannula 16 is allowed to shift from the collapsed position to the expanded position and therefore extends in a direction that is not parallel with the artery 502 or the body of the catheter 10. In this manner, as shown in FIGS. 8C and 8D, the proximal end 20 of the projection cannula 16 is directed through the opening formed in the arterial wall 502 by the introducer 504.

[0075] Accordingly, when the catheter 10 is positioned within the artery 502, the antegrade blood arterial blood flow is allowed to continue through the artery 502 through the proximal end 12 of the catheter 10, while only a portion of the arterial blood is rerouted through the projection

cannula 16 and into the veins 506 of interest. In this manner, the normal blood flow through the artery 502 is not inhibited by operation of the autoretroperfusion system 100. Furthermore, in addition to bifurcating the blood flowing through the artery 502, the projection cannula 16 traversing the arterial wall 502 further functions to anchor the catheter 10 in the desired position within the artery 502.

[0076] In the example where the catheter 10 further comprises the expandable balloon 58 (see FIG. 1), step 404 may further comprise inflating the expandable balloon 58 to the desired size by injecting fluid into the balloon port 62. In this manner, the expandable balloon 58 functions to further anchor the catheter 10 in the desired location within the artery 502 and seal the opening in the artery 502 through which the projection cannula 16 projects (see FIG. 8E).

[0077] At step 406, a vein 506 of interest is percutaneously punctured under local anesthesia with a conventional venous access device or as otherwise known in the art. For example and without limitation, in at least one example, an 18 gauge needle is inserted into the femoral or subclavian vein. At step 408, a delivery catheter 508 is inserted into and advanced through the vein 506 to catheterize the coronary sinus ostium. A guidewire 510 is then inserted at step 410 into the delivery catheter 510 and advanced into the lumen of the vein 506 through the distal end of the delivery catheter 510. Furthermore, the guidewire 510 is advanced into the region of interest by use of x-ray (i.e. fluoroscopy), direct vision, transesophageal echocardiogram, or other suitable means or visualization techniques.

[0078] FIGS. 9 and 10 show schematic views of the method 400 as applied to a heart 500. Specifically, in this at least one example, at steps 402 and 404 the artery 502, which in FIG. 9 comprises the subclavian artery, is punctured and the catheter 10 is inserted and positioned therein. Further, at step 406 the vein 506, which in FIG. 9 comprises the subclavian vein, is punctured and at step 408 the delivery catheter 508 is advanced through the superior vena cava 518 and into the coronary ostium of the coronary sinus 520. As shown in FIG. 10, at step 410, the guidewire 510 is advanced through the coronary sinus 520 and into the vein of interest, which, in this at least one example, comprises the posterior vein 522 of the heart 500.

[0079] Now referring back to FIG. 7, the guidewire 510 inserted into the vein 506 at step 410 may further comprise a plurality of impedance electrodes as previously described herein. In this approach, the guidewire 510 may be used at optional step 411 to determine the size of the vessel of interest through use of the plurality of impedance electrodes disposed thereon. In this manner, a clinician can use the measurements generated by the impedance electrodes to select a properly sized expandable balloon 158 for use in connection with the second catheter 150. By using a precisely sized expandable balloon 158 and inflation volume, the clinician can ensure that the distal end 154 of the second catheter 150 is securely anchored within the vessel of interest without imposing an undue force on the venous vessel walls.

[0080] After the guidewire 510 has been advanced into the vessel of interest at step 410 and, optionally, the dimensions of the vessel of interest have been measured at step 411, the method 400 advances to step 412. At step 412, the distal end 154 of the second catheter 150 is inserted into the delivery catheter 508 over the guidewire 510. Accordingly, the guidewire 510 is slidably received by the at least one lumen 156 of the second catheter 150. The distal end 154 of the second catheter 150 is then advanced over the guidewire 510 to the region of interest and the expandable balloon 158 of the second catheter 150 is inflated to anchor the distal end 154 within the targeted vessel. FIG. 11 shows a schematic view of the method 400, as applied to the heart 500, after step 412 has been completed. It will be understood that at any point after the distal end 154 of the second catheter 150 is positioned and anchored within the desired location in the targeted vessel, the delivery catheter 508 and the guidewire 510 may be withdrawn from the vein of interest.

[0081] After the distal end 154 of the second catheter 150 is secured within the targeted vessel, at step 414 the anastomosis between the vein 506 and the artery 502 is formed. Specifically, in at least one approach, the proximal end 20 of the projection cannula 16 of the catheter 10 is coupled with the proximal end 152 of the second catheter 150 by way of the connector 170. In the at least one example of the system 100 comprising the first graft 185 and the second graft 190, the connector 170 may be coupled with the catheter 10 and the second catheter 150 via the first graft 185 and the second graft 190 to form an elongated anastomosis. Alternatively, in yet another approach, the connector 185 may be coupled with the catheter 10 via the proximal end 20 of the projection cannula 16 and the second catheter 150 via only the second graft 190. It will be understood that any combination of the catheter 10, the second catheter 150 and the first and second grafts 185, 190 may be used in connection with the connector 170 to form the desired anastomosis between the vein 506 and the artery 502.

[0082] After the anastomosis is formed and the arterial blood is allowed to flow through the anastomosis and thereby through the connector 170, at step 416 the connector 170 measures the flow rate, pressure and any other desired data of the arterial blood flow. The connector 170 transmits the collected data to the remote module 180 either through intravascularly placed leads or wirelessly, through telemetry or other means. In this manner, a clinician may easily view the blood flow data on the remote module 180 and assess the degree of pressure drop that will be required to preserve and gradually arterialize the vein 506.

[0083] At step 418, the pressure of the arterial blood flow through the system 100 is modified to transmit the desired pressure to the venous system. In this step 418 the pressure modification can be achieved through a cli-

nician modifying the means of regulating the blood flow of the connector 170 through remote means or, in at least one example of the system 100, inflating the internal expandable balloon of the second catheter 150 using the internal balloon port in order to partially occlude the flow of arterial blood through the at least one lumen 156 of the second catheter 150. Furthermore, in at least one alternative example of the system 100, a clinician may deliver a resorbable stenosis configured to achieve the necessary pressure drop into the at least one lumen 156 of the second catheter 150 through means known in the art.

[0084] Alternatively, as previously described in connection with autoretroperfusion system 100, the remote module 180 may further comprise a computer or other processing means capable of being programmed to automatically analyze the data received from the connector 170 and, based on such data, determine the proper degree of adjustment required in the blood pressure flowing through the anastomosis. In this example, at step 418, the remote module 180 automatically adjusts the means of regulating the blood flow of the connector 170 to achieve the optimal pressure drop. In this manner, the desired pressure drop between the arterial system and the venous system is immediately achieved and the risk of venous rupture is significantly reduced.

[0085] In step 420 the method 400 allows the arterial blood having a modified pressure to irrigate the vein 506 for a period of time such that the vein 506 properly arterializes. For example, and without limitation, the patient's venous system may be subjected to the reduced arterial pressure for about fourteen days to allow the vein 506 to adapt to the elevated blood pressure flowing therethrough.

[0086] After arterialization of the vein 506 is achieved, at step 422 the patient may optionally undergo a coronary venous bypass graft surgery and the components of the autoretroperfusion system 100 may be removed. However, as previously discussed, even with a properly arterialized vein 506, many patients that require retroperfusion therapy may still not be candidates for a coronary vein bypass graft surgery. In the event that the patient is unable to tolerate such a procedure, after the vein 506 has arterialized at step 420, the method 400 can progress directly to step 424. At step 424, the pressure modification of the arterial blood flowing through the second catheter 150 is ceased. Accordingly, pre-arterialized veins 506 are subjected to the full arterial pressure of the blood flowing through the anastomosis and second catheter 150. In at least one example, a clinician can cease the pressure modification by adjusting the controller 170. Alternatively, in the at least one example where the controller 170 can be automatically adjusted by the remote module 180, the remote module 180 can automatically adjust the controller 170 after the veins 506 have pre-arterialized. Further, where the pressure drop is achieved through the use of an internal expandable balloon positioned within the at least one lumen 156 of the second catheter, the clinician may deflate the internal expandable balloon through the internal balloon port and thereafter withdraw the deflated internal expandable balloon through the tertiary lumen of the second catheter and the internal balloon port. In yet another example where a resorbable stenosis is used to achieve the pressure drop in the arterial blood as it flows through the second catheter 150, the resorbable stenosis can be configured to dissolve after the desired period of time, thereby gradually decreasing the influence the resorbable stenosis has on the pressure of the blood flowing through the at least one lumen 156 of the second catheter over a period of time. Accordingly, the autoretroperfusion system 100 can remain chronically implanted within the patient to deliver oxygen-rich blood to a targeted area of tissue over an extended period of time.

[0087] Now referring to FIG. 12, a flow chart of a method 600 for performing simultaneous selective retroperfusion using the SSA system 300 is shown. While the method 600 is described herein in connection with treating a heart 500 through catheterization of the coronary sinus 520, it will be understood that the method 600 may be used to perform autoretroperfusion on any organ or tissue in need of retroperfusion treatment. The reference numerals used to identify the steps of method 600 that are included in the description of method 400 designate like steps between the two methods 400, 600. As such, like steps between the two methods 400, 600 will not be discussed in detail with respect to the method 600 and it will be understood that such description can be obtained through the description of the method 400.

[0088] Method 600, and the examples thereof, can be performed under local anesthesia and does not require arterial sutures. Further, once implanted, the SSA system 300 can deliver simultaneous chronic treatment to multiple ischemic locations as the system 300 is capable of remaining within a patient's vascular system for an extended period of time and selectively retroperfusion more than one sub-branch of a vein 506.

[0089] The method 600 progresses through steps 402 through 410 as previously described in connection with the method 400. After the guidewire 510 is advanced through the coronary sinus 520 and into the first vein of interest, a second guidewire 610 is inserted at step 602 into the delivery catheter 508 adjacent to the guidewire 510, and advanced into the lumen of the vein 506 through the distal end of the delivery catheter 510. The second guidewire 610 is then advanced into a second region of interest by use of x-ray (i.e. fluoroscopy), direct vision, transesophageal echocardiogram, or other suitable means or visualization techniques. The second guidewire 610 is configured similar to the guidewire 510 and is capable of functioning the in the same manner.

[0090] FIG. 13 shows a schematic view of the method 600 as applied to a heart 500. Specifically, in this at least one example, FIG. 13 shows the method 600 at step 602 wherein the guidewire 510 is inserted a first vein of interest, which comprises the posterior vein 522 of the heart

500, and the second guidewire 610 is inserted into a second vein of interest, which comprises the interventricular vein 622 of the heart 500.

[0091] Now referring back to FIG. 12, the guidewire 610 inserted into the second vein of interest in step 602 may further comprise a plurality of impedance electrodes as previously described with respect to the guidewire 510. In this example, the guidewire 610 may be used at optional step 603 to determine the size of the second vessel of interest through use of the plurality of impedance electrodes disposed thereon. In this manner, a clinician can use the measurements generated by the impedance electrodes to select a properly sized expandable balloon 358 for use in connection with the third catheter 350. By using a precisely sized expandable balloon 358 and inflation volume, a clinician can ensure that the distal end 354 of the third catheter 350 is securely anchored within the second vessel of interest without imposing an undue force on the venous vessel walls.

[0092] After the guidewire 610 has been advanced into the second vessel of interest at step 602 and, optionally, the dimensions of the second vessel of interest have been measured at step 603, the method 600 advances to step 412 wherein the second catheter 150 is inserted over the guidewire 510 as described in connection with method 400. At step 604, the distal end 354 of the third catheter 350 is inserted into the delivery catheter 508 over the second guidewire 610. Accordingly, the second guidewire 610 is slidably received by the at least one lumen 356 of the third catheter 350. The distal end 354 of the third catheter 350 is then advanced over the second guidewire 610 to the second region of interest and the expandable balloon 358 of the third catheter 350 is inflated to anchor the distal end 354 within the targeted vessel. FIG. 14 shows a schematic view of the method 600 at step 604 as applied to the heart 500. It will be understood that at any point after the distal ends 154, 354 of the second and third catheters 150, 350 are positioned and anchored in the desired locations within the targeted vessels, the delivery catheter 508 and the guidewires 510, 610 may be withdrawn from the vein 506.

[0093] After both the distal end 154 of the second catheter 150 and the distal end 354 of the third catheter 350 are secured within the targeted vessels, the method 600 proceeds to step 414 where the anastomosis is formed between the vein 506 and the artery 502 as described in connection with method 400. Thereafter, the method 600 advances through steps 416 through 424 as described in connection with the method 400. Furthermore, at step 418, it will be recognized that a clinician can independently adjust the pressure drop through the second and third catheters 150, 350 in the event that an internal expandable balloon is used in either or both catheters 150, 350 or resorbable stenosis are employed within the at least one lumens 156, 356 of the second and third catheters 150, 350. Alternatively, in the at least one example where the controller 170 comprises a means for regulating the blood flow through the anastomosis, the pressure of the arterial blood flowing through both the second and third catheters 150, 350 may be substantially the same.

[0094] As described herein, the method 600 may be used to simultaneously and immediately treat two different ischemic areas of a tissue through the use of one minimally to non-invasive procedure. Furthermore, the method 600 can provide no-option patients with a viable treatment option that is not associated with contraindications for congestive heart failure, diabetes, or drug treatment.

[0095] While various embodiments of devices and systems for achieving autoretroperfusion of the heart tissue have been described in considerable detail herein, the embodiments are merely offered by way of non-limiting examples of the disclosure described herein. Many variations and modifications of the embodiments described herein will be apparent to one of ordinary skill in the art in light of this disclosure. It will therefore be understood by those skilled in the art that various changes and modifications may be made, and equivalents may be substituted for elements thereof, without departing from the scope of the disclosure. Indeed, this disclosure is not intended to be exhaustive or to limit the scope of the disclosure. The scope of the disclosure is to be defined by the appended claims, and by their equivalents.

[0096] Further, in describing representative examples, the description may have presented a method and/or process as a particular sequence of steps. However, to the extent that the method or process does not rely on the particular order of steps set forth herein, the method or process should not be limited to the particular sequence of steps described. As one of ordinary skill in the art would appreciate, other sequences of steps may be possible.

Claims

1. A catheter (10) for controlling blood perfusion pressure, the catheter (10) comprising:

an elongated body configured for placement within an artery, the elongated body having a proximal open end (12), a distal open end (14), and at least one lumen (15) extending between the proximal open end (12) and the distal open end (14);

a cannula (16) configured to extend through an opening in the artery and to extend from the elongated body such that an angle is formed therebetween, the cannula (16) comprising a hollow interior having a first diameter in fluid communication with at least one lumen (15), the at least one lumen (15) having a second diameter, wherein the first diameter is less than the second diameter, **characterised in that**

the cannula (16) is movable between a substantially extended configuration wherein the angle

comprises between about 15° and about 90° and a substantially collapsed configuration wherein the angle comprises less than about 15°, wherein the distal open end (14) of the elongated body is configured to receive a fluid flowing through the artery and the proximal open end (12) is configured to allow the fluid received by the distal open end (14) of the elongated body to flow therethrough; and the cannula is configured to route a portion of the fluid received by the distal open end (14) of the elongated body outside of the artery, to modify the pressure of fluid flowing through the cannula, in use.

2. The catheter (10) of claim 1, wherein the cannula (16) is biased towards the substantially extended configuration.

3. The catheter (10) of claim 1, further comprising an expandable balloon (58) coupled with the elongated body.

4. The catheter (10) of claim 3, further comprising a balloon port (62) in fluid communication with the expandable balloon (58) through a secondary lumen (60) of the catheter (10).

5. The catheter (10) of claim 4, wherein the balloon port (62) is configured for subcutaneous implantation.

6. The catheter (10) of claim 1, wherein the hollow interior of the cannula (16) comprises a diameter having a value between about 2.7 millimeters to about 4 millimeters.

7. The catheter (10) of claim 1, wherein the cannula (16) is hingedly movable between the substantially extended configuration and the substantially collapsed configuration

8. A system (100) for controlling blood perfusion pressure within a vein, the system comprising:

a first catheter (10) according to any preceding claim configured for placement within an arterial vessel,
a second catheter (150) configured for placement within a venous vessel, the second catheter (150) having a proximal end (152), a distal end (154), and at least one lumen (156) extending between the proximal end (152) and the distal end (154); and
a connector (170) coupled with the cannula (16) of the first catheter (10) and the proximal end (152) of the second catheter (150), the connector (170) comprising:

a means for measuring data associated with fluid flowing therethrough, and
a means for automatically regulating blood flow based on the data measured by the means for measuring data.

9. The system (100) of claim 8, wherein the first catheter (10) has an expandable balloon (58) coupled with the elongated body and the expandable balloon (58) is configured to prevent fluid leakage through the arterial opening when the expandable balloon (58) is in a substantially inflated configuration and the elongated body of the first catheter (10) is positioned within an arterial vessel such that the cannula (16) extends through the arterial opening.

10. The system (100) of claim 8, wherein the second catheter (150) comprises an expandable balloon (158) coupled with the exterior of the second catheter (50).

11. The system (100) of claim 8, further comprising a first graft (185) coupled with the proximal end (152) of the second catheter (150) and the connector (170) such that the at least one lumen (156) of the second catheter (150) is in fluid communication with the at least one lumen (15) of the first catheter (10).

12. The system (100) of claim 11, further comprising a second graft (190) coupled with the cannula (16) of the first catheter (10) and the connector (170) such that the at least one lumen (156) of the second catheter (150) is in fluid communication with the at least one lumen (15) of the first catheter (10).

Patentansprüche

1. Katheter (10) zum Steuern eines Blutperfusionsdrucks, wobei der Katheter (10) aufweist:

einen länglichen Körper, der zu einem Platzieren innerhalb einer Arterie konfiguriert ist, wobei der längliche Körper ein nahes offenes Ende (12), ein fernes offenes Ende (14) und zumindest ein Lumen (15), das sich zwischen dem nahen offenen Ende (12) und dem fernen offenen Ende (14) erstreckt, hat,
eine Hohlnadel (16), die konfiguriert ist, um sich durch eine Öffnung in der Arterie zu erstrecken und um sich von dem länglichen Körper zu erstrecken, so dass ein Winkel dazwischen gebildet ist, wobei die Hohlnadel (16) ein hohles Inneres, das einen ersten Durchmesser hat, in Fluidkommunikation mit zumindest einem Lumen (15) aufweist, wobei das zumindest eine Lumen (15) einen zweiten Durchmesser hat,
wobei der erste Durchmesser geringer als der zweite Durchmesser ist, **gekennzeichnet da-**

durch, dass
die Hohlnadel (16) zwischen einer im Wesentlichen erstreckten Konfiguration, wobei der Winkel zwischen ungefähr 15° und ungefähr 90° aufweist, und einer im Wesentlichen zusammengefallenen Konfiguration, wobei der Winkel weniger als ungefähr 15° aufweist, bewegbar ist, wobei das ferne offene Ende (14) des länglichen Körpers konfiguriert ist, um ein Fluid, das durch die Arterie strömt, zu erhalten, und das nahe offene Ende (12) konfiguriert ist, um dem Fluid, das durch das ferne offene Ende (14) des länglichen Körpers erhalten wird, zu erlauben, dort durchzuströmen, und die Hohlnadel konfiguriert ist, um einen Teil des Fluids, das durch das ferne offene Ende (14) des länglichen Körpers erhalten wird, aus der Arterie zu leiten, um bei Verwendung den Druck des durch die Hohlnadel strömenden Fluids zu modifizieren.

2. Katheter (10) nach Anspruch 1, wobei die Hohlnadel (16) in Richtung der im Wesentlichen erstreckten Konfiguration vorgespannt ist.

3. Katheter (10) nach Anspruch 1, der außerdem einen ausdehnbaren Ballon (58) aufweist, der mit dem länglichen Körper gekoppelt ist.

4. Katheter (10) nach Anspruch 3, der außerdem einen Ballonanschluss (62) aufweist, der durch ein zweites Lumen (60) des Katheters (10) in Fluidkommunikation mit dem ausdehnbaren Ballon (58) steht.

5. Katheter (10) nach Anspruch 4, wobei der Ballonanschluss (62) für subkutane Implantierung konfiguriert ist.

6. Katheter (10) nach Anspruch 1, wobei das hohle Innere der Hohlnadel (16) einen Durchmesser, der einen Wert zwischen ungefähr 2,7 Millimeter bis ungefähr 4 Millimeter hat, aufweist.

7. Katheter (10) nach Anspruch 1, wobei die Hohlnadel (16) zwischen der im Wesentlichen erstreckten Konfiguration und der im Wesentlichen zusammengefallenen Konfiguration schwenkbar bewegbar ist.

8. System (100) zu einem Steuern eines Blutperfusionsdrucks innerhalb einer Vene, wobei das System aufweist:

einen ersten Katheter (10) nach einem vorherigen Anspruch, der zu einem Platzieren innerhalb eines arteriellen Gefäßes konfiguriert ist,
einen zweiten Katheter (150), der zu einem Platzieren innerhalb eines venösen Gefäßes konfiguriert ist, wobei der zweite Katheter (150) ein nahes Ende (152), ein entferntes Ende (154) und zumindest ein Lumen (156), das sich zwischen dem nahen Ende (152) und dem entfernten Ende (154) erstreckt, hat, und
einen Verbinder (170), der mit der Hohlnadel (16) des ersten Katheters (10) und dem nahen Ende (152) des zweiten Katheters (150) gekoppelt ist, wobei der Verbinder (170) aufweist:

eine Einrichtung zu einem Messen von Daten, die mit dem dort durchströmenden Fluid assoziiert sind, und
eine Einrichtung zum automatischen Regulieren des Blutstroms auf Grundlage der Daten, die durch die Einrichtung zum Messen von Daten gemessen wurden.

9. System (100) nach Anspruch 8, wobei der erste Katheter (10) einen ausdehnbaren Ballon (58), der mit dem länglichen Körper gekoppelt ist, hat und der ausdehnbare Ballon (58) konfiguriert ist, um eine Fluidleckage durch die arterielle Öffnung zu verhindern, wenn der ausdehnbare Ballon (58) in einer im Wesentlichen aufgeblasenen Konfiguration ist und der längliche Körper des ersten Katheters (10) innerhalb eines arteriellen Gefäßes positioniert ist, so dass die Hohlnadel (16) sich durch die arterielle Öffnung erstreckt.

10. System (100) nach Anspruch 8, wobei der zweite Katheter (150) einen ausdehnbaren Ballon (158), der mit dem Äußeren des zweiten Katheters (50) gekoppelt ist, aufweist.

11. System nach Anspruch 8, das außerdem ein erstes Transplantat (185) aufweist, das mit dem nahen Ende (152) des zweiten Katheters (150) und dem Verbinder (170) gekoppelt ist, so dass das zumindest eine Lumen (156) des zweiten Katheters (150) in Fluidkommunikation mit dem zumindest einen Lumen (15) des ersten Katheters (10) ist.

12. System nach Anspruch 11, das außerdem ein zweites Transplantat (190) aufweist, das mit der Hohlnadel (16) des ersten Katheters (10) und dem Verbinder (170) gekoppelt ist, so dass das zumindest eine Lumen (156) des zweiten Katheters (150) in Fluidkommunikation mit dem zumindest einen Lumen (15) des ersten Katheters (10) ist.

Revendications

1. Cathéter (10) pour contrôler la pression d'une perfusion sanguine, le cathéter (10) comprenant :

un corps allongé configuré pour le placement à l'intérieur d'une artère, le corps allongé ayant une extrémité ouverte proximale (12), une ex-

trémité ouverte distale (14), et au moins une lumière (15) s'étendant entre l'extrémité ouverte proximale (12) et l'extrémité ouverte distale (14) ;
une canule (16) configurée pour s'étendre à travers une ouverture dans l'artère et pour s'étendre à partir du corps allongé de telle sorte qu'un angle est formé entre eux, la canule (16) comprenant un intérieur creux ayant un premier diamètre en communication fluidique avec au moins une lumière (15), l'au moins une lumière (15) ayant un second diamètre,
dans lequel le premier diamètre est inférieur au second diamètre, **caractérisé en ce que**
la canule (16) est mobile entre une configuration sensiblement étendue dans laquelle l'angle comprend entre environ 15° et environ 90° et une configuration sensiblement repliée dans laquelle l'angle comprend moins de 15° environ, dans lequel l'extrémité ouverte distale (14) du corps allongé est configurée pour recevoir un fluide s'écoulant à travers l'artère et l'extrémité ouverte proximale (12) est configurée pour permettre au fluide reçu par l'extrémité ouverte distale (14) du corps allongé de s'écouler à travers elle ; et la canule est configurée pour acheminer une partie du fluide reçu par l'extrémité ouverte distale (14) du corps allongé hors de l'artère, pour modifier le pression de fluide s'écoulant à travers la canule, en utilisation.

2. Cathéter (10) selon la revendication 1, dans lequel la canule (16) est sollicitée vers la configuration sensiblement étendue.

3. Cathéter (10) selon la revendication 1, comprenant en outre un ballonnet dilatable (58) couplé au corps allongé.

4. Cathéter (10) selon la revendication 3, comprenant en outre un orifice de ballonnet (62) en communication fluidique avec le ballonnet dilatable (58) à travers une lumière secondaire (60) du cathéter (10).

5. Cathéter (10) selon la revendication 4, dans lequel l'orifice de ballonnet (62) est configuré pour une implantation sous-cutanée.

6. Cathéter (10) selon la revendication 1, dans lequel l'intérieur creux de la canule (16) comprend un diamètre ayant une valeur comprise entre environ 2,7 millimètres et environ 4 millimètres.

7. Cathéter (10) selon la revendication 1, dans lequel la canule (16) est mobile de manière articulée entre la configuration sensiblement étendue et la configuration sensiblement repliée.

8. Système (100) pour contrôler une pression de perfusion sanguine à l'intérieur d'une veine, le système comprenant :

un premier cathéter (10) selon l'une quelconque des revendications précédentes configuré pour le placement à l'intérieur d'un vaisseau artériel, un second cathéter (150) configuré pour le placement à l'intérieur d'un vaisseau veineux, le second cathéter (150) ayant une extrémité proximale (152), une extrémité distale (154), et au moins une lumière (156) s'étendant entre l'extrémité proximale (152) et l'extrémité distale (154) ; et
un raccord (170) couplé à la canule (16) du premier cathéter (10) et à l'extrémité proximale (152) du second cathéter (150), le raccord (170) comprenant :

un moyen pour mesurer des données associées au fluide s'écoulant à travers lui, et un moyen pour réguler automatiquement le flux sanguin sur la base des données mesurées par le moyen pour mesurer les données.

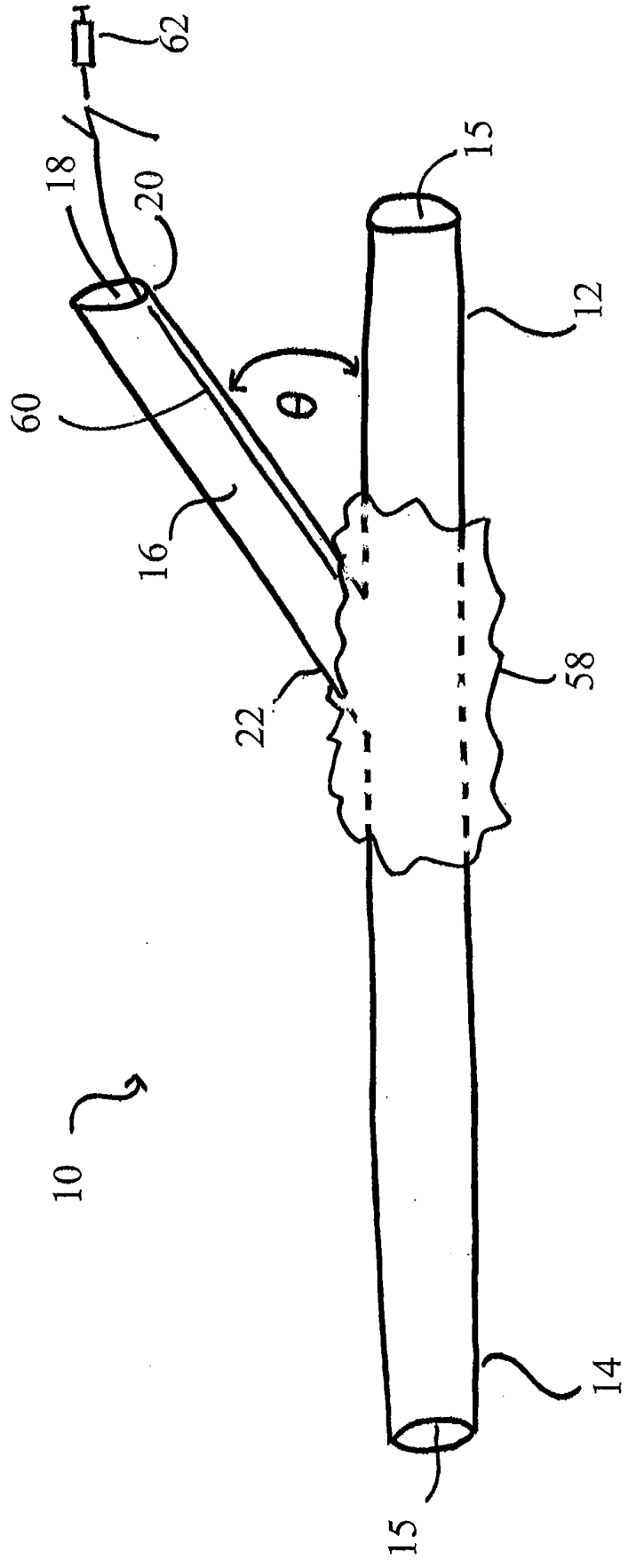
9. Système (100) selon la revendication 8, dans lequel le premier cathéter (10) a un ballonnet dilatable (58) couplé au corps allongé et le ballonnet dilatable (58) est configuré pour empêcher la fuite de fluide à travers l'ouverture artérielle lorsque le ballonnet dilatable (58) est dans une configuration sensiblement gonflée et le corps allongé du premier cathéter (10) est positionné à l'intérieur d'un vaisseau artériel de telle sorte que la canule (16) s'étend à travers l'ouverture artérielle.

10. Système (100) selon la revendication 8, dans lequel le second cathéter (150) comprend un ballonnet dilatable (158) couplé avec l'extérieur du second cathéter (50).

11. Système (100) selon la revendication 8, comprenant en outre un premier greffon (185) couplé à l'extrémité proximale (152) du second cathéter (150) et au raccord (170) de telle sorte que l'au moins une lumière (156) du second cathéter (150) est en communication fluidique avec l'au moins une lumière (15) du premier cathéter (10).

12. Système (100) selon la revendication 11, comprenant en outre un second greffon (190) couplé à la canule (16) du premier cathéter (10) et au raccord (170) de telle sorte que l'au moins une lumière (156) du second cathéter (150) est en communication fluidique avec l'au moins une lumière (15) du premier cathéter (10).

FIG. 1



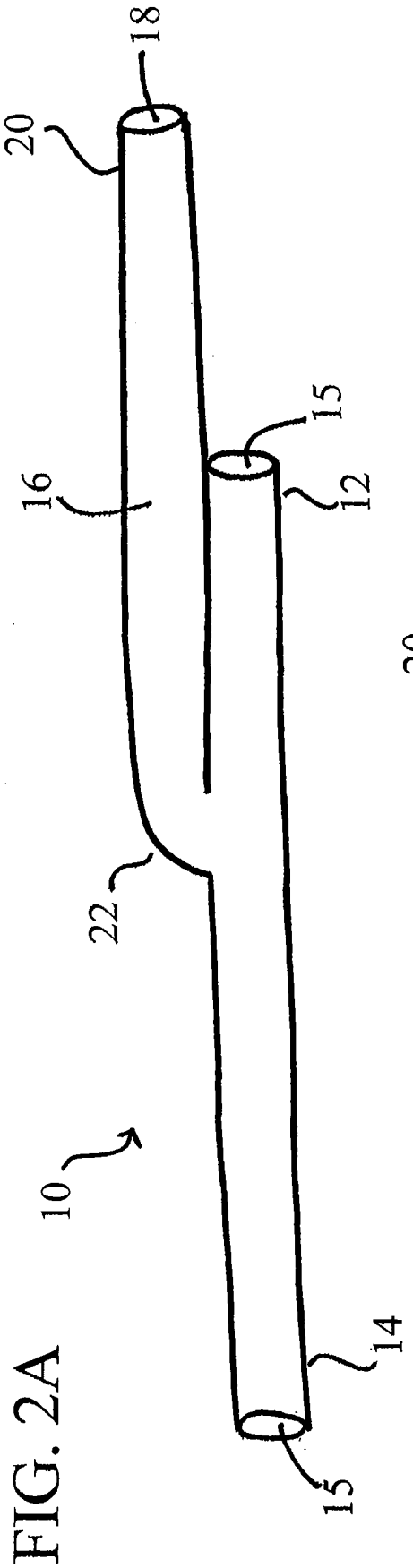


FIG. 2A

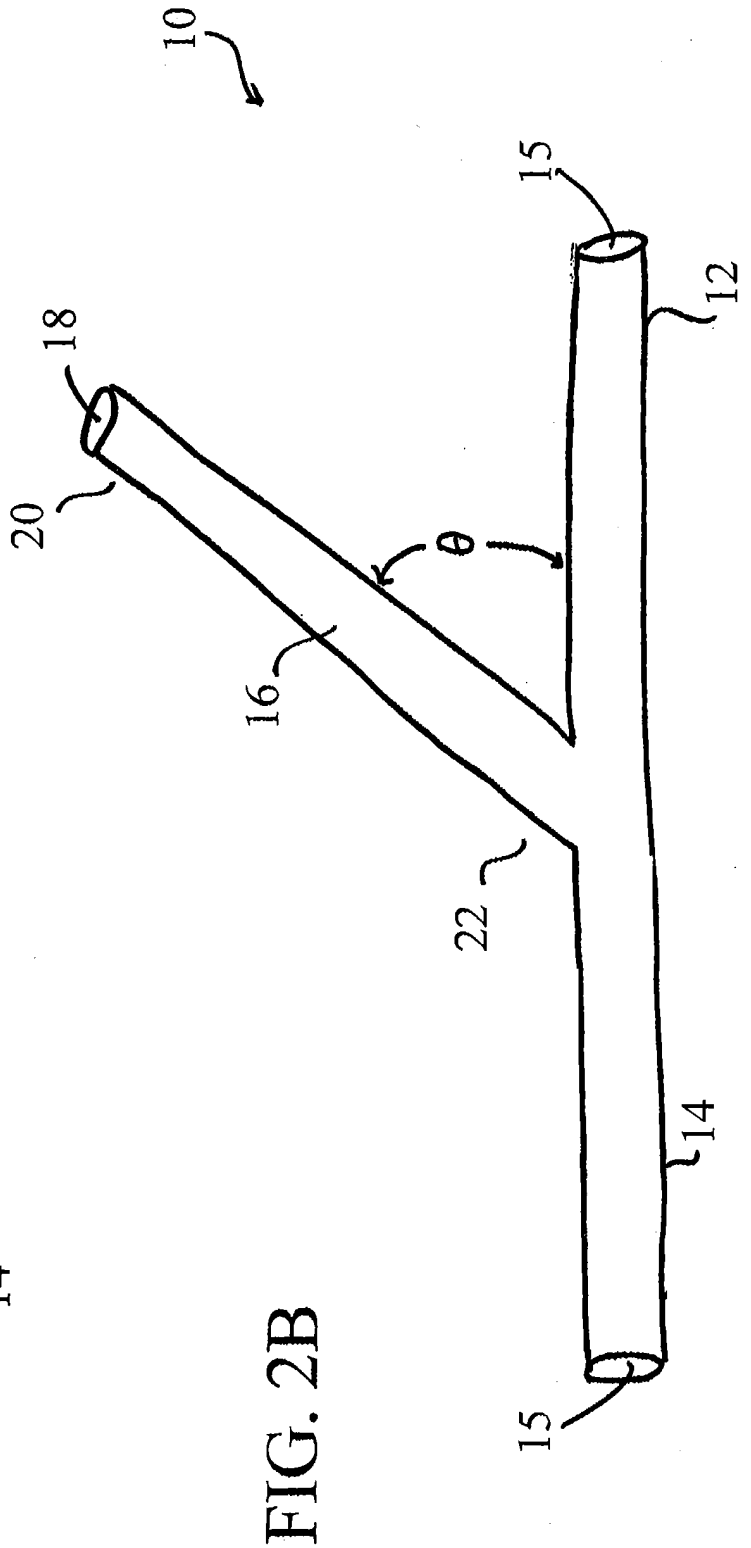


FIG. 2B

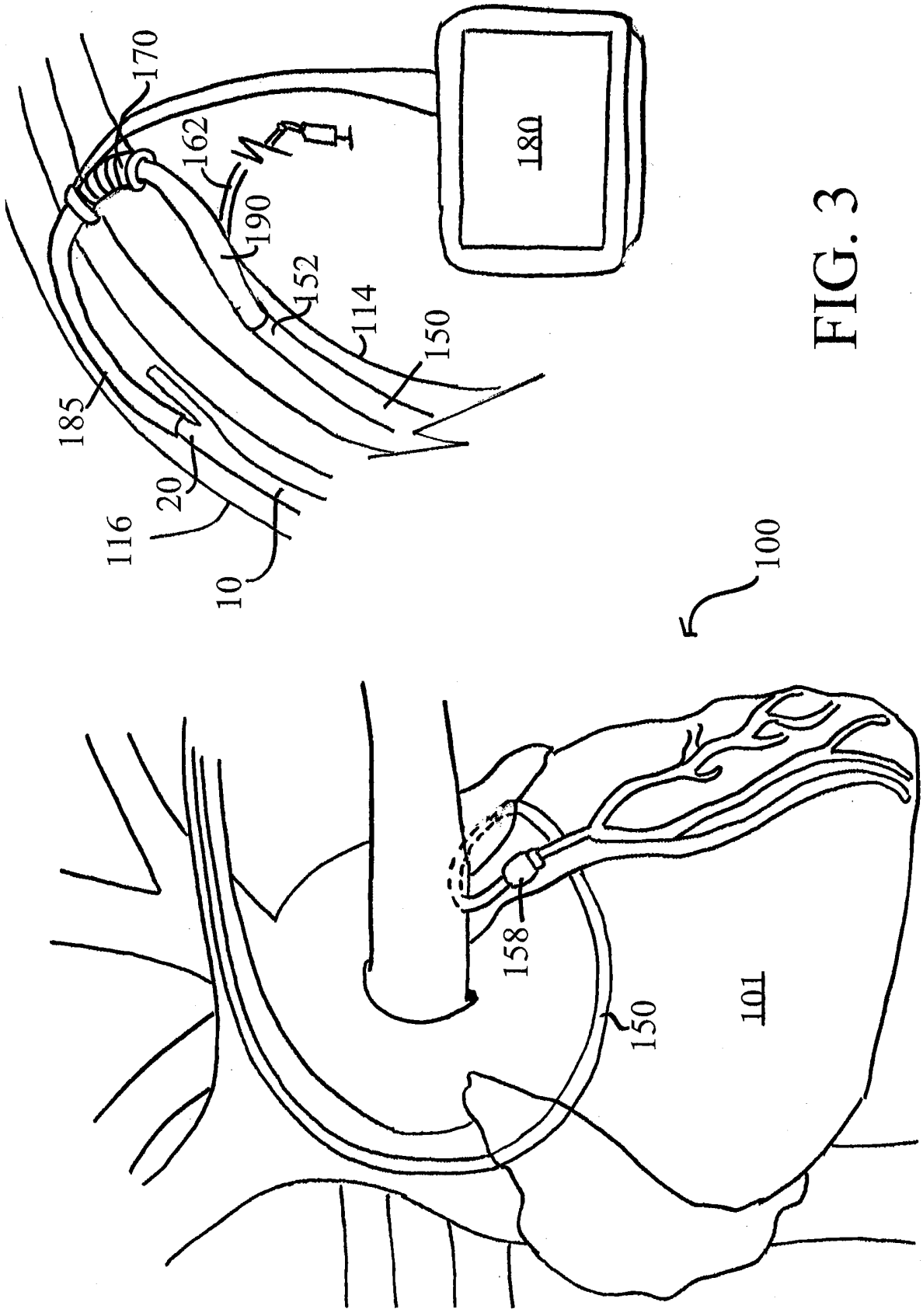


FIG. 3

FIG. 4B

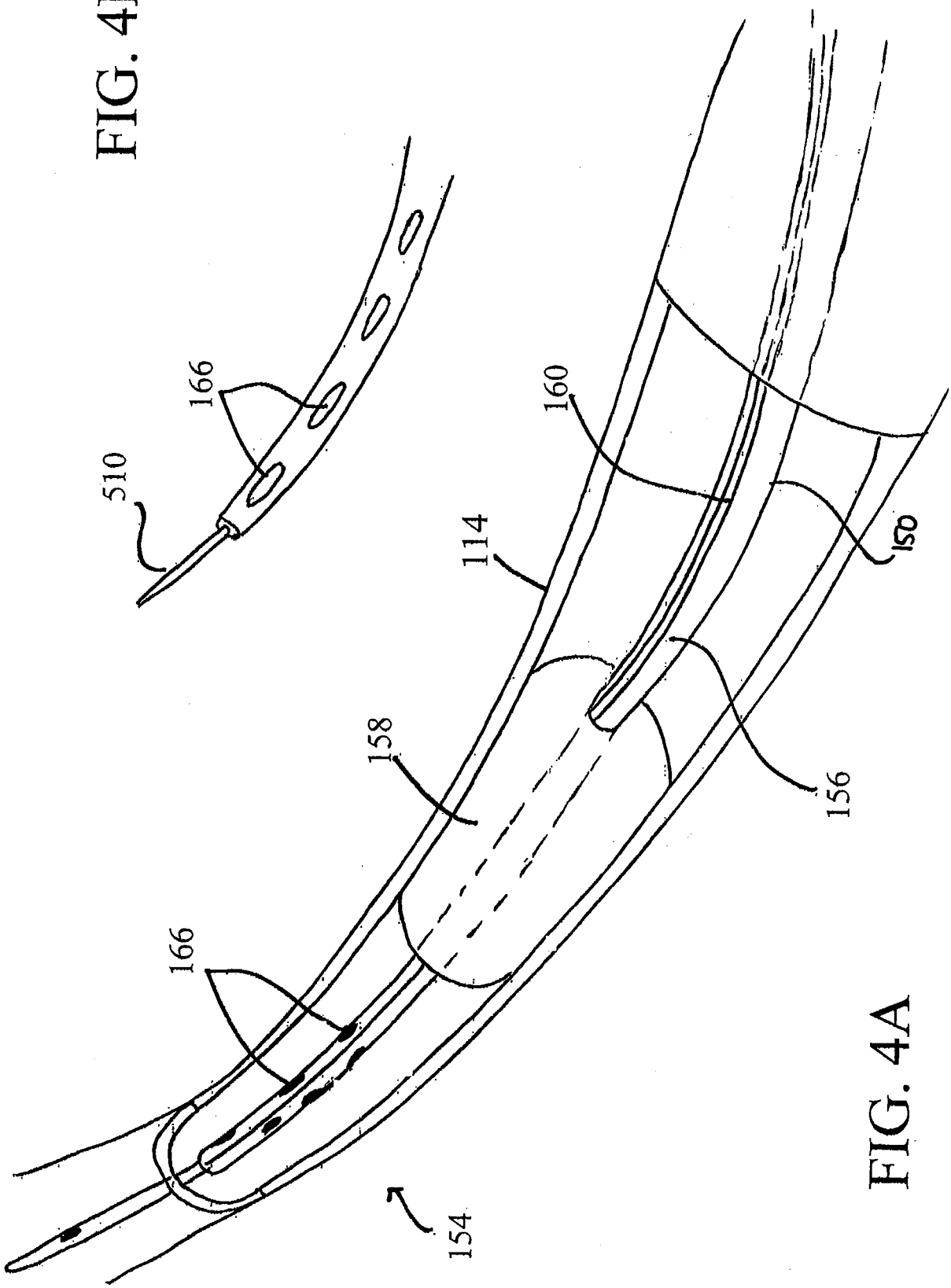
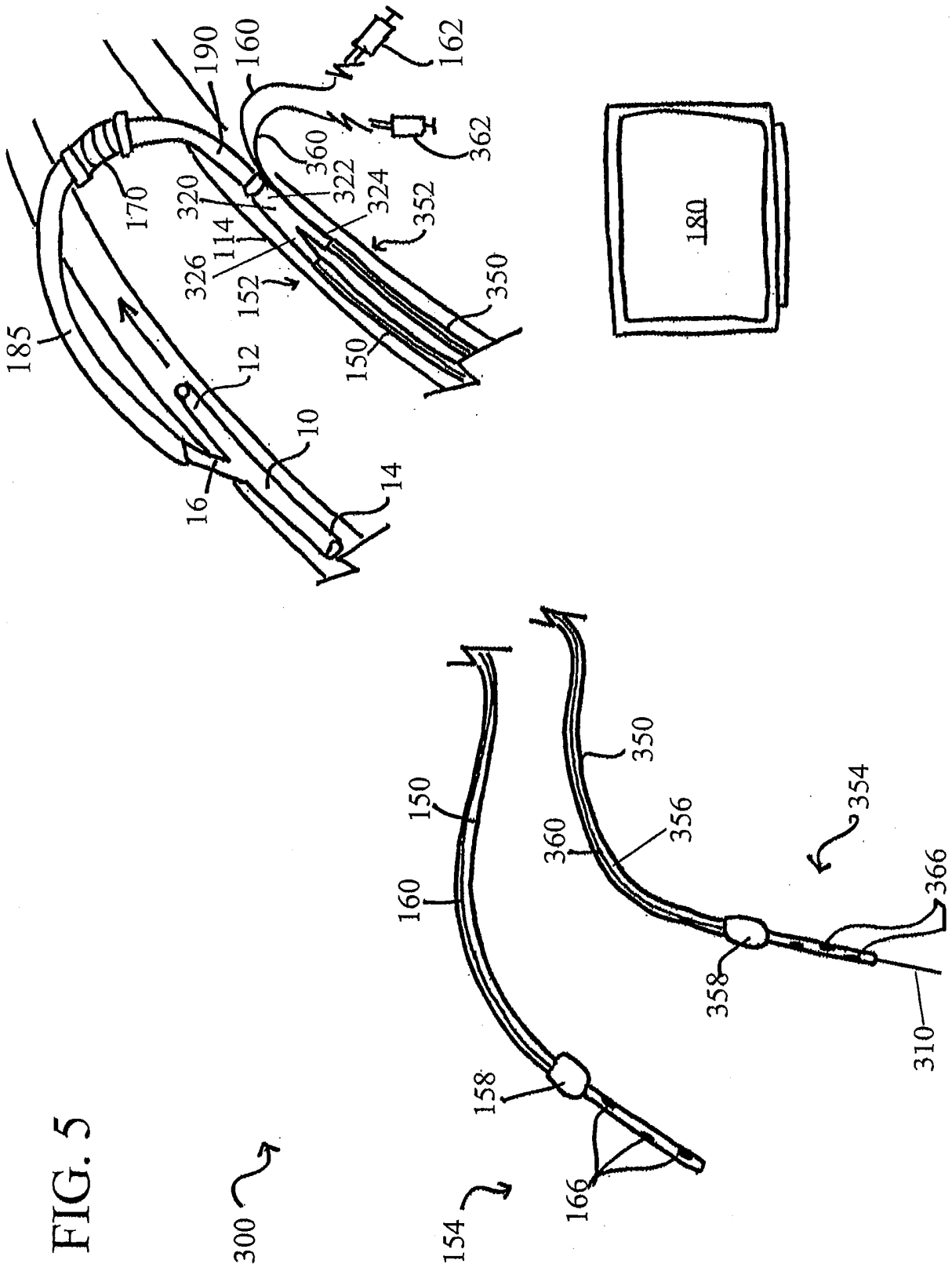


FIG. 4A

FIG. 5


300
185
190
160
162
170
320
360
322
324
362
352
326
114
152
350
150
12
10
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14
180
154
158
166
150
160
350
360
356
354
366
358
310

FIG. 6

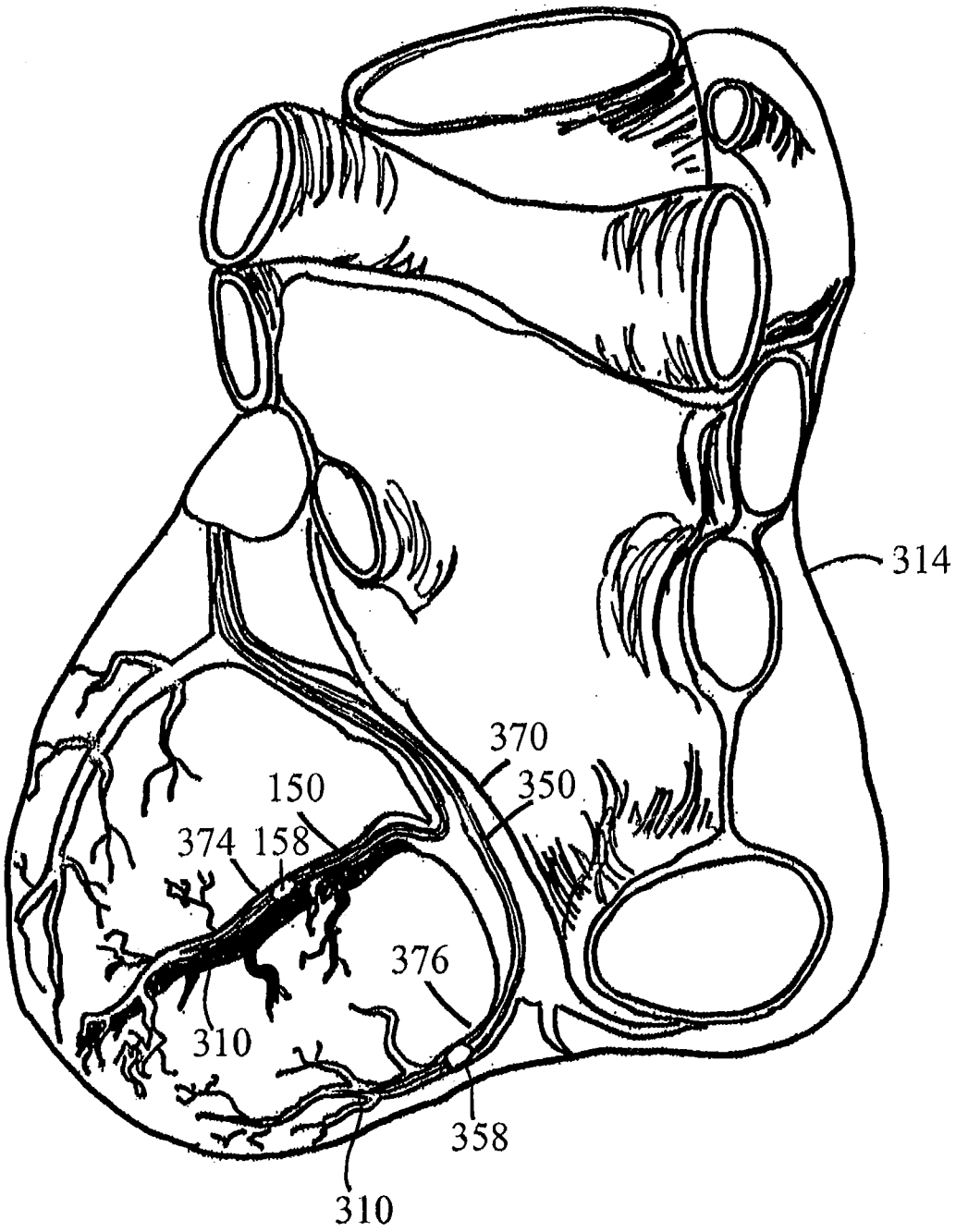


FIG. 7

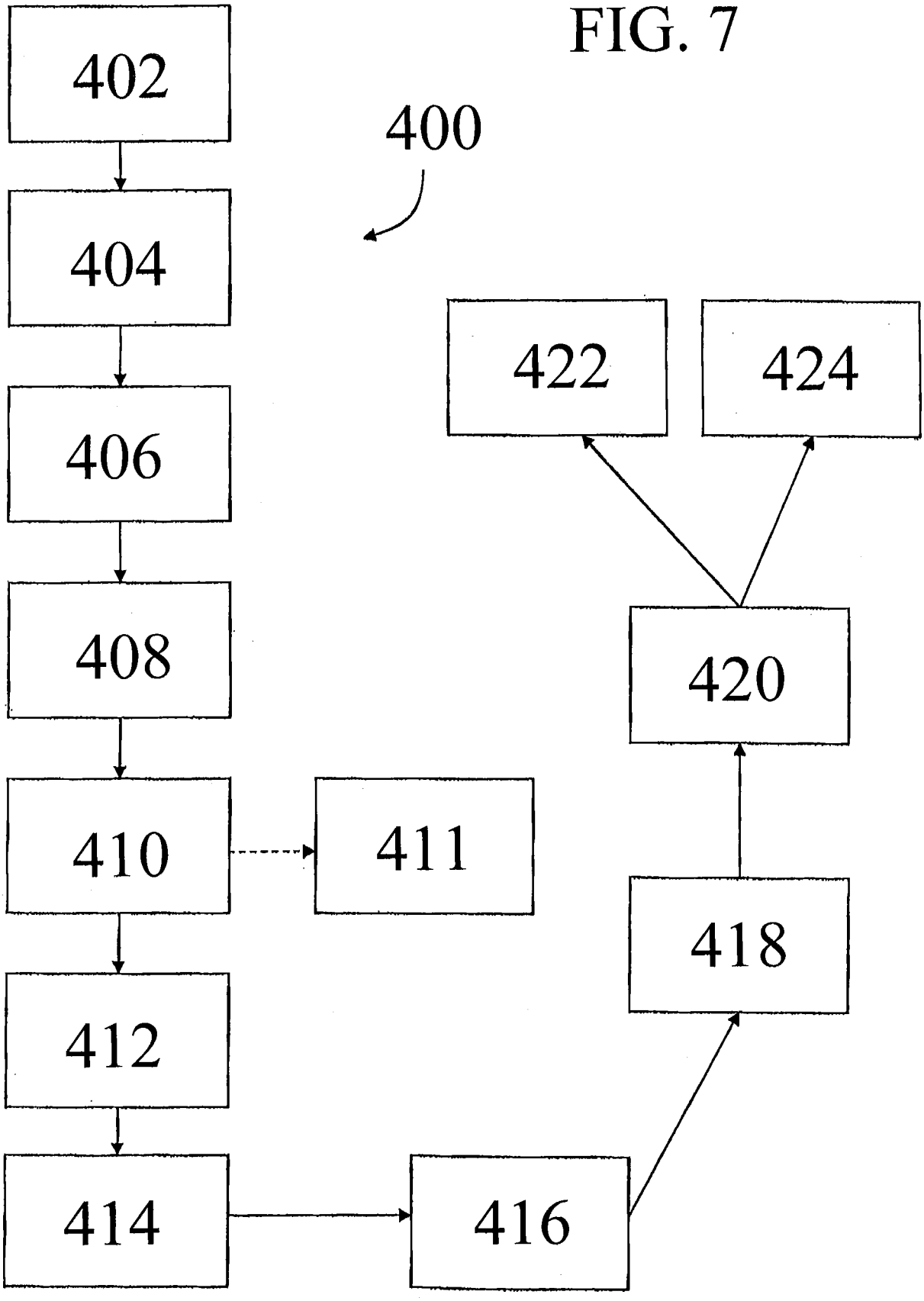


FIG. 8A

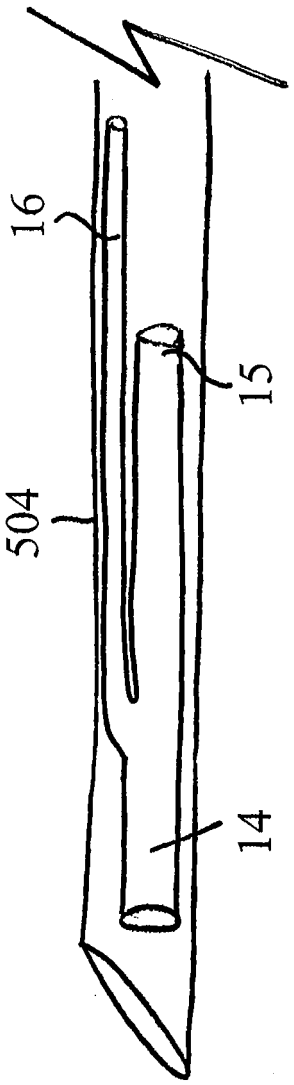


FIG. 8B

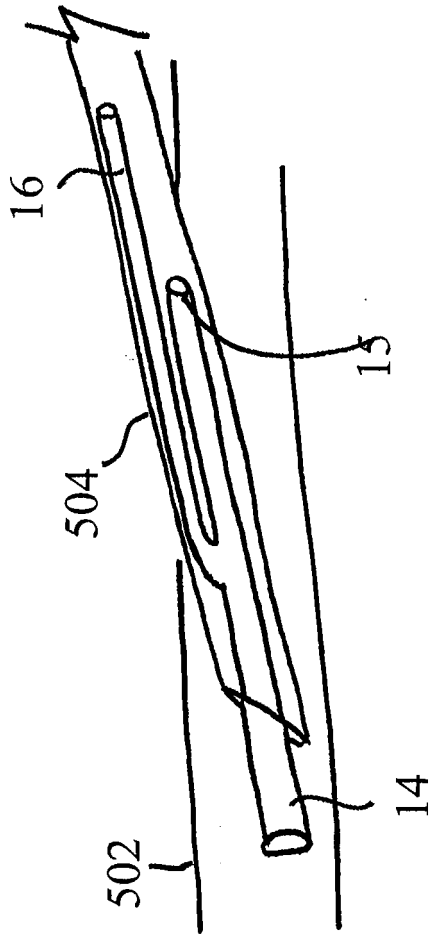


FIG. 8C

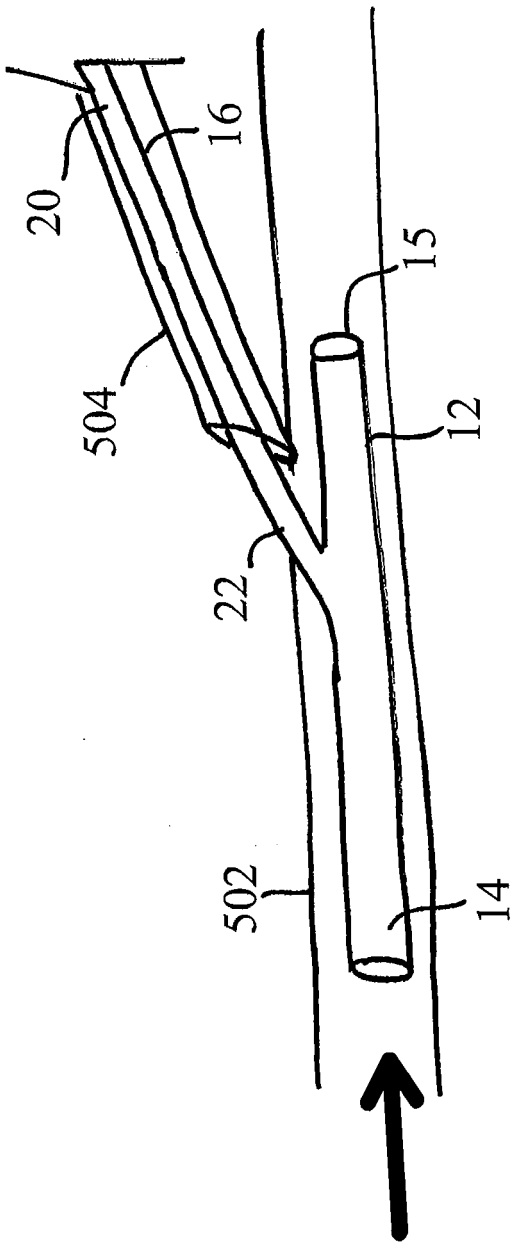
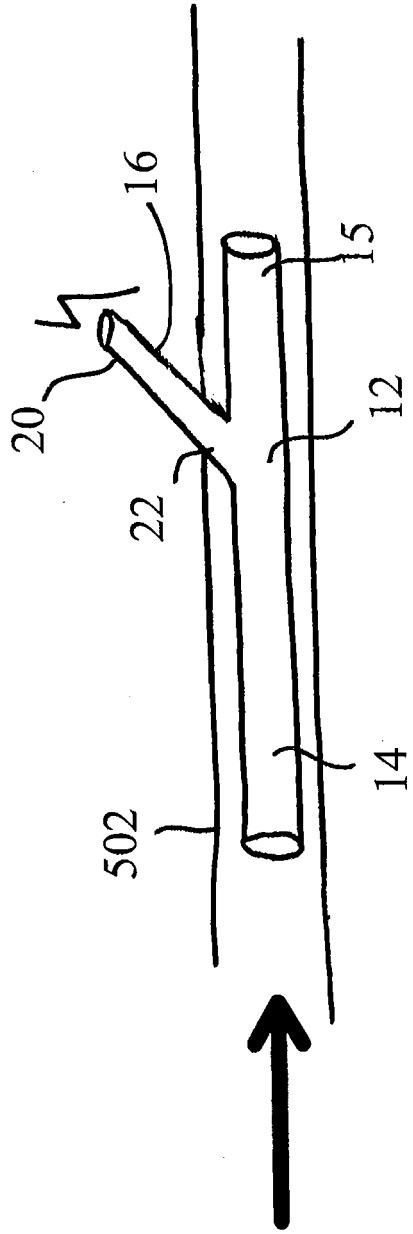


FIG. 8D



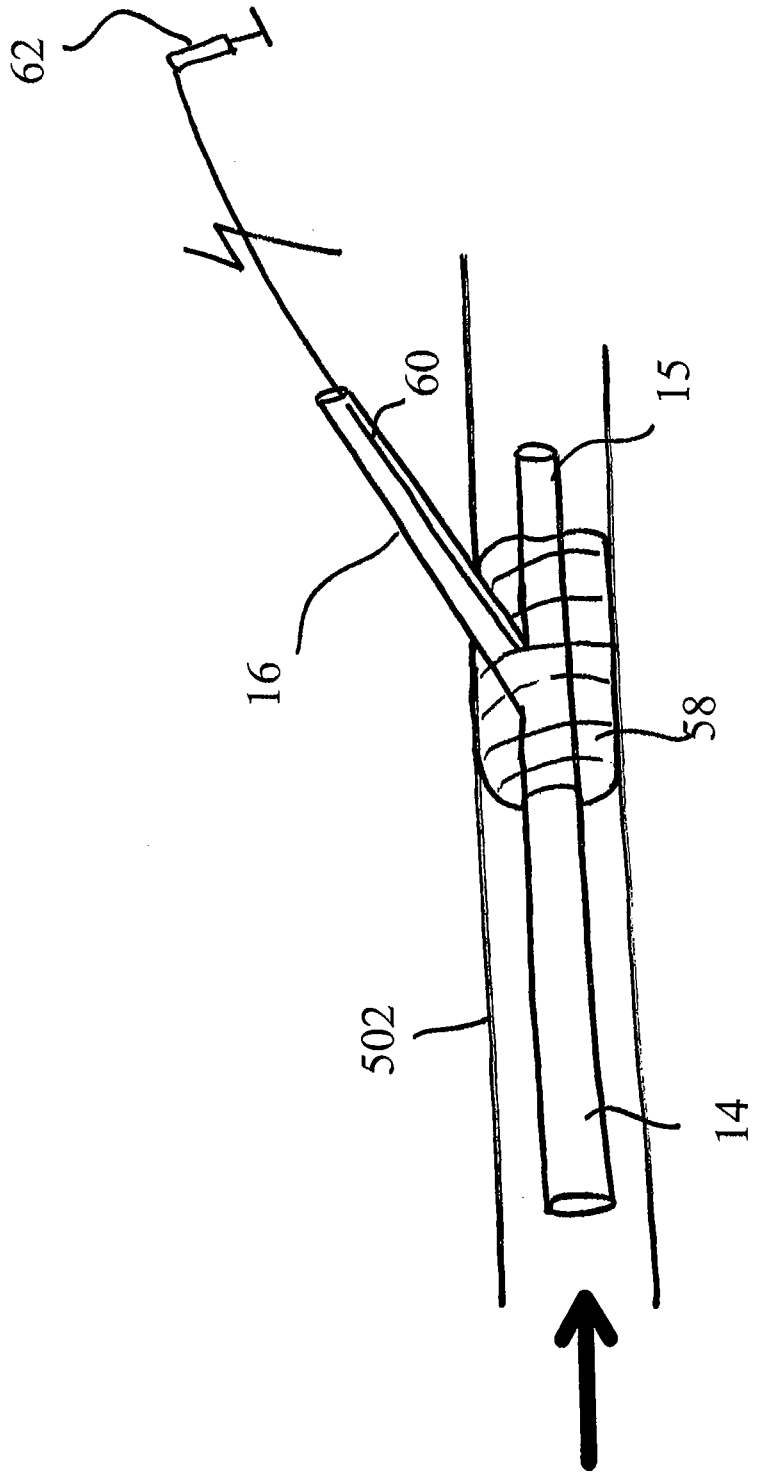


FIG. 8E

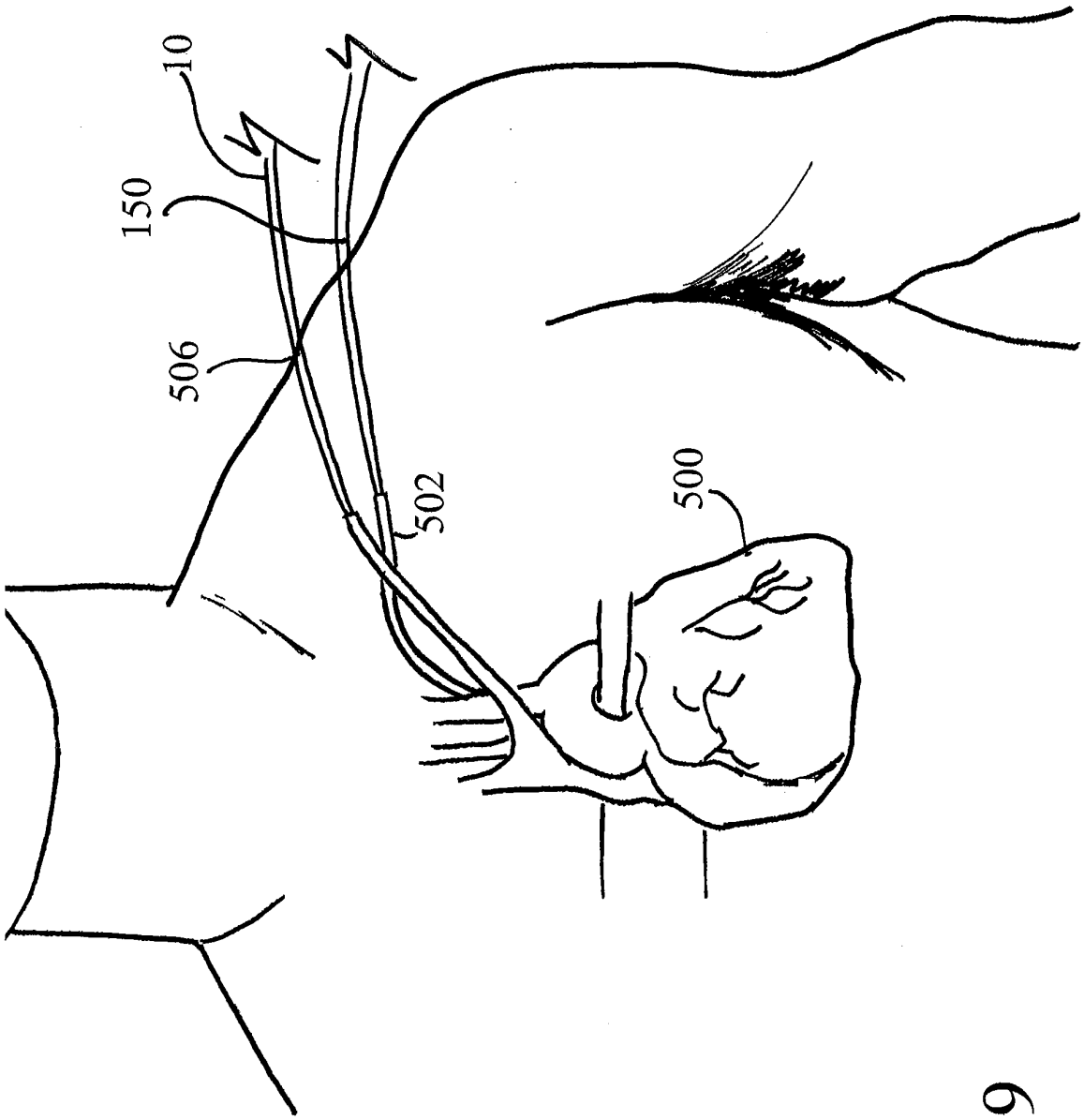


FIG. 9

FIG. 10

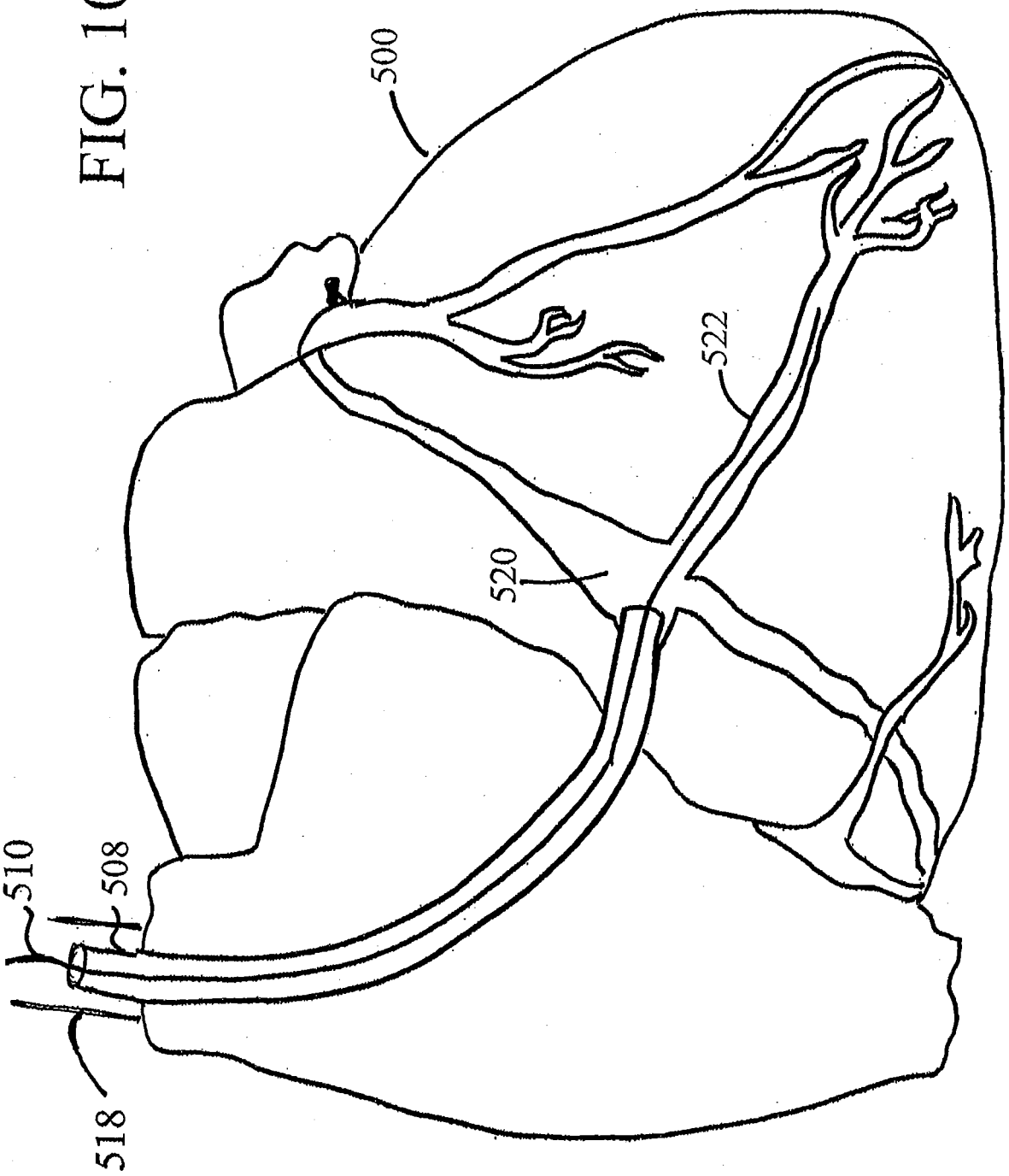


FIG. 11

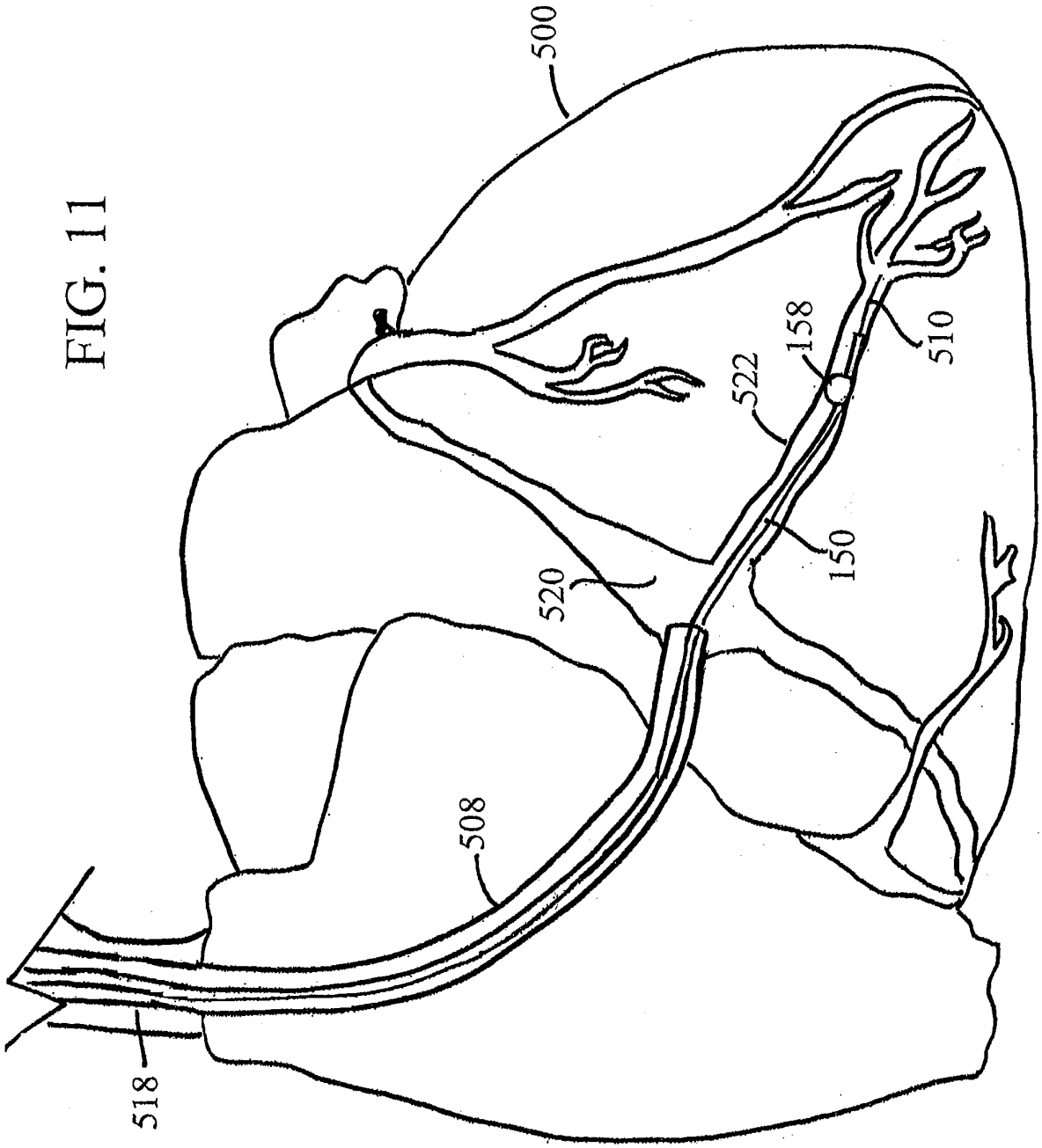


FIG. 12

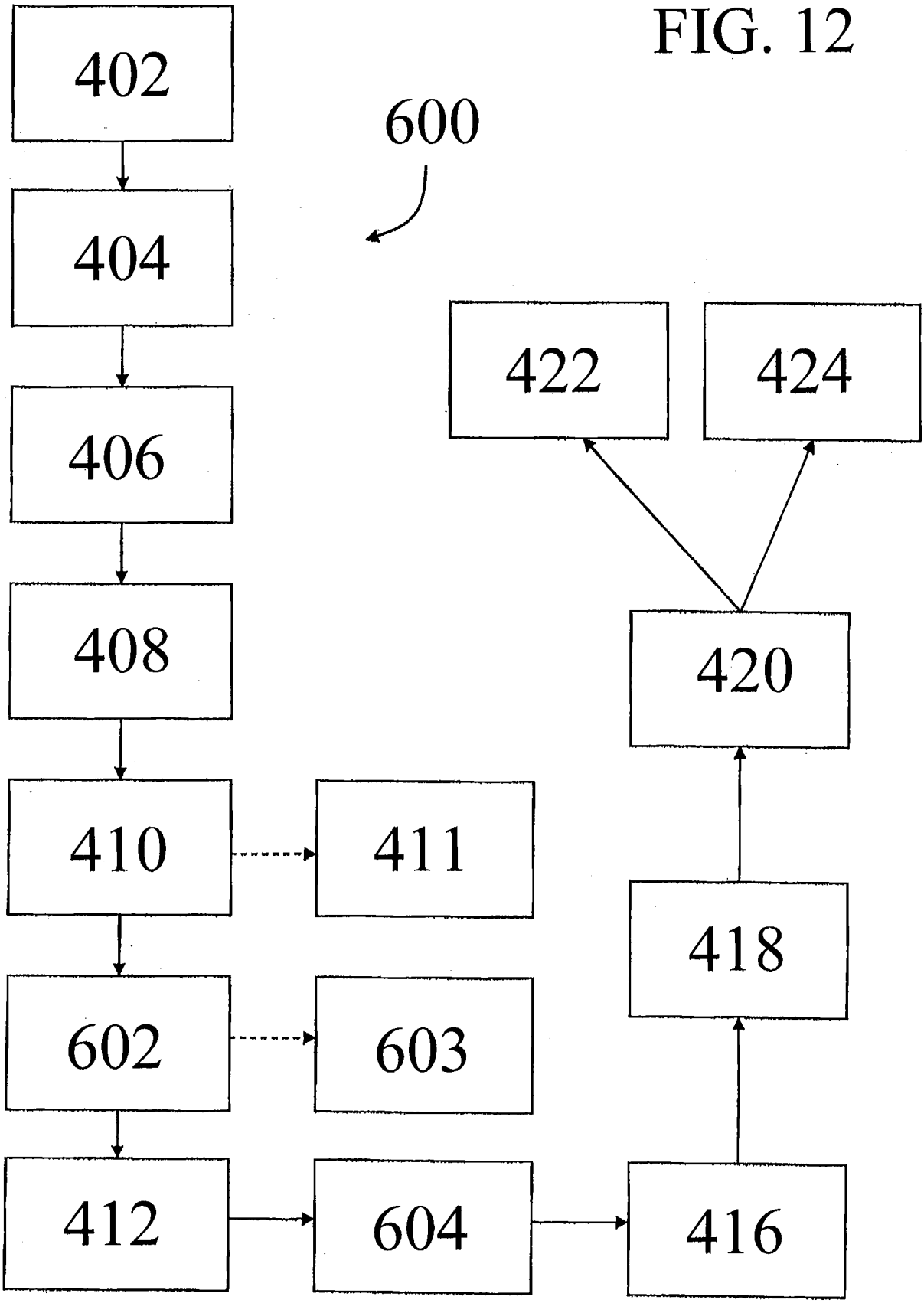


FIG. 13

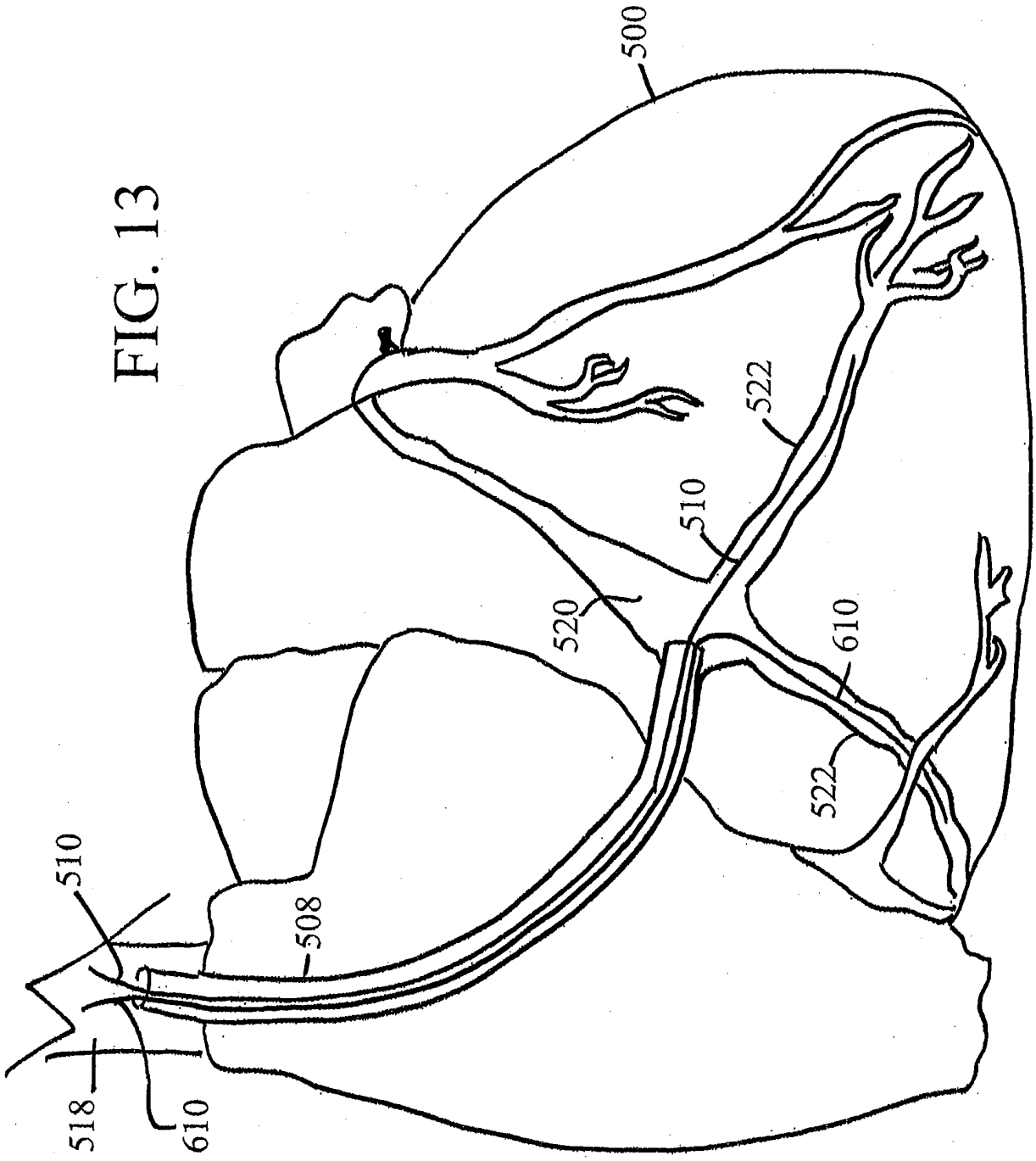
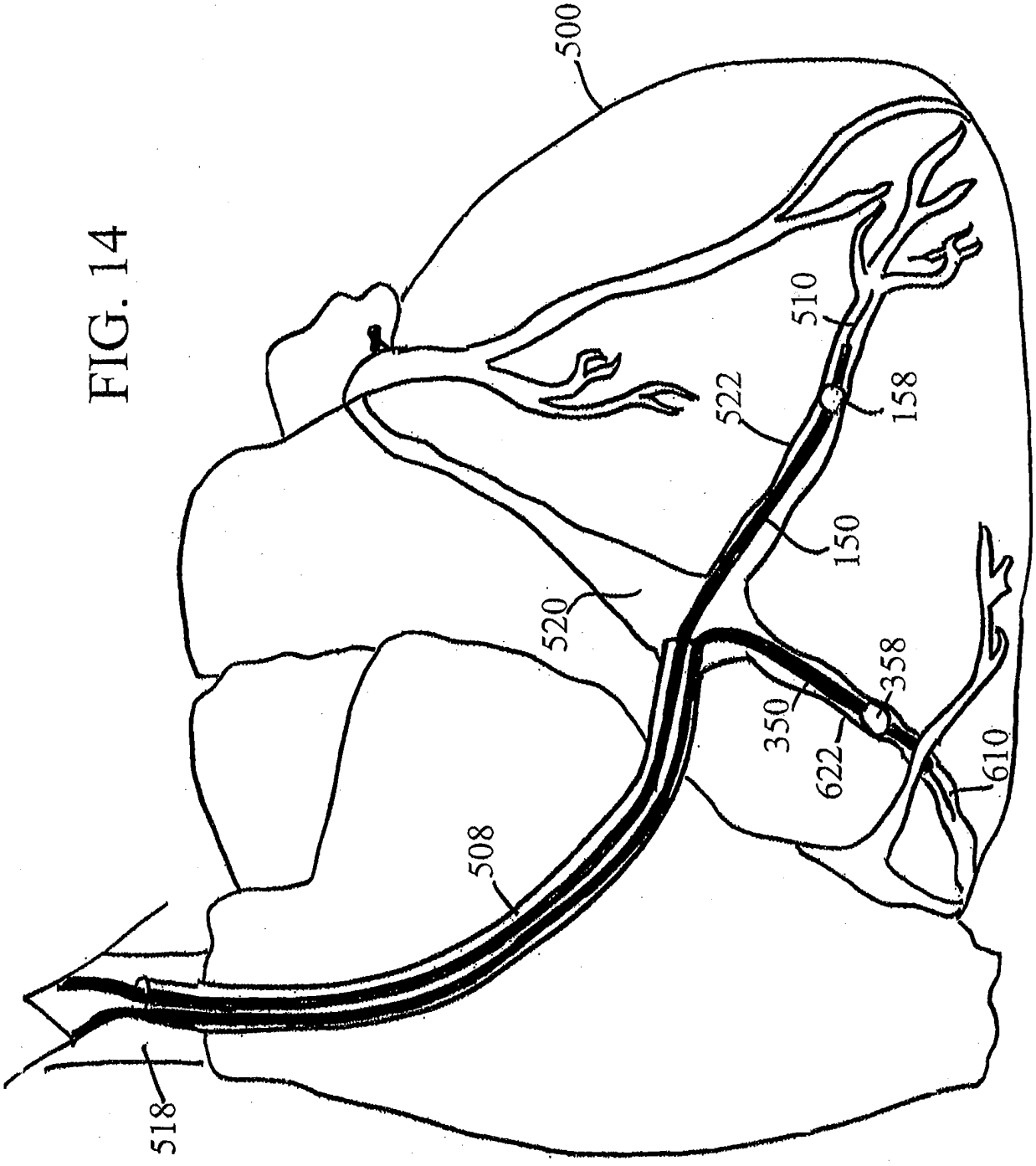


FIG. 14



REFERENCES CITED IN THE DESCRIPTION

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- US 2006029223 W **[0047]**
- US 10782149 B **[0059]**

专利名称(译)	用于实现静脉动脉化的自动灌注装置，系统和方法		
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摘要(译)

公开了用于以微创方式向至少一个缺血组织提供逆向灌注的装置，系统和方法。本文公开的至少一些实施例使得能够在不使用缝线和通过非侵入性手术的情况下在静脉和动脉之间形成吻合。另外，各种公开的实施例提供了一种套管装置，其包括Y形构造，用于在吻合术和下方动脉之间分叉动脉血流。本文的装置，系统和方法可以进一步向缺血组织的一个以上区域提供同时自动反流灌注治疗。