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(54) **ATRIAL FIBRILLATION DETECTION SYSTEM**

ERKENNUNGSSYSTEM FÜR VORHOFFLIMMERN

SYSTÈME DE DÉTECTION DE FIBRILLATION AURICULAIRE

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- **JÜRGEN R. SCHAEFER ET AL: "Improved Detection of Paroxysmal Atrial Fibrillation Utilizing a Software-Assisted Electrocardiogram Approach", PLOS ONE, vol. 9, no. 2, 28 February 2014 (2014-02-28), page e89328, XP055278473, DOI: 10.1371/journal.pone.0089328**

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Description**TECHNICAL FIELD**

[0001] The present invention relates to an atrial fibrillation detection system.

BACKGROUND ART

[0002] Atrial fibrillation refers to a condition in which the atria twitch finely and cannot contract sufficiently, due to irregular and rapid stimulation throughout the atria. Meanwhile, since some stimulation of the atria travels through the atrioventricular node, the ventricles contract at irregular intervals, irrespective of the sinus rhythm. Thus, because the ventricles contract, albeit irregularly, and there is no marked loss of coronary function, many people fail to notice the symptoms of atrial fibrillation. It is estimated that there are about 1,000,000 patients suffering from atrial fibrillation within Japan, but it is thought that if people who fail to notice the symptoms were included, the number of patients would be far greater.

[0003] Since, the atria cannot contract sufficiently under atrial fibrillation, blood tends to pool within the atria, producing clots, leading to the possibility that such a clot may be transported to the brain, causing a cerebral infarction. Therefore, patients with atrial fibrillation are said to be about five times more likely to have a cerebral infarction than individuals without symptoms.

[0004] Because blood clots produced by atrial fibrillation are large in size, in many instances large blood vessels of the brain become obstructed. For this reason, a cerebral infarction that is caused by atrial fibrillation can inflict wide-ranging damage to the brain, making a prognosis that the individual will be left with an impediment severe enough to require nursing care highly likely. Nursing care may impose physical, psychological, and economic burdens on the family providing assistance, and is thought to impose a large economic burden on society as well.

[0005] While full recovery from atrial fibrillation may prove possible by reducing clot formation through the administration of drugs, or by catheter ablation, early detection is necessary to do so. However, as mentioned above, atrial fibrillation in many cases does not produce subjective symptoms. Moreover, in paroxysmal cases, the disorder may not be discovered by an EKG exam during a routine checkup or hospital visit.

[0006] Research has been carried out with the goal of using the heartbeat period to distinguish atrial fibrillation. For example, one such method involves calculating the distribution of the difference ΔR in adjacent heartbeat periods for a healthy individual and an atrial fibrillation patient, respectively, and automatically detecting atrial fibrillation by the Kolmogorov-Smirnov test. However, this method requires that heartbeat period values be taken over an extended period in order to obtain the ΔR distribution, imposing a burden on the test subjects. Moreover, it is possible that paroxysmal atrial fibrillation occurring within a brief time interval will not be detected.

[0007] Another method distinguishes atrial fibrillation based on a standard deviation obtained from a heartbeat period distribution (Patent Document 1). However, the technique disclosed in Patent Document 1 also requires heartbeat periods to be calculated, and therefore requires that heartbeat period values be taken over an extended period.

[0008] A further method distinguishes the condition through frequency analysis of heartbeat period fluctuations (Patent Document 2), but requires heartbeat period values measured continuously over several minutes for the purpose of frequency analysis, and it is possible that paroxysmal atrial fibrillation will not be detected.

[0009] Patent Document 3 discloses a computer implemented method for discriminating between atrial fibrillation and premature ventricular contractions and premature atrial contractions.

[Related Art Documents]

[Patent Documents]

[0010]

[Patent Document 1] Japanese Laid-open Patent Application 2009-89883

[Patent Document 2] Japanese Laid-open Patent Application 2013-55982

[Patent Document 3] US 2014/0330134 A1

SUMMARY OF THE INVENTION PROBLEMS THE INVENTION IS INTENDED TO SOLVE

[0011] With the foregoing in view, it is an object of the present invention to provide a novel atrial fibrillation detection system with which it is possible to detect (symptoms of) atrial fibrillation using only heartbeat period values measured over a brief time period, so that the burden on the test subject can be reduced, and with which it is possible to detect

even paroxysmal atrial fibrillation; and moreover to accomplish this using a compact measuring device for measuring only heartbeat periods of the heart, thus making use in the home possible, and contributing to early detection of atrial fibrillation.

MEANS FOR SOLVING THESE PROBLEMS

[0012] A summary of the present invention will be described with reference to the accompanying drawings.

[0013] The present invention relates to an atrial fibrillation detection system for detecting the presence of atrial fibrillation in a subject, wherein the atrial fibrillation detection system is characterized by being provided with heartbeat period measurement means that measures heartbeat periods of the heart; normalized heartbeat period computation means that computes normalized heartbeat periods $DR(N)$, represented by the following equation (1), where R_n is a time series of heartbeat periods of the heart, from heartbeat periods of the heart that were measured by the heartbeat period measurement means; abnormal normalized heartbeat period cumulation means that, from among a prescribed number of successive normalized heartbeat periods $DR(N)$, adds up the count of abnormal normalized heartbeat periods that have an absolute value exceeding a normal heartbeat period value; and comparison/determination means that compares the cumulative count of the abnormal normalized heartbeat periods and a normal cumulative count threshold value, and in the event that the cumulative count of the abnormal normalized heartbeat periods exceeds the normal cumulative count threshold value, determines that atrial fibrillation has occurred.

$$DR(N)_n = \frac{N(R_{n-1} - R_n)}{\sum_{k=n-N+1}^n R_k} \quad \dots\dots (1)$$

N is an integer greater than 1, subscript n is a time series, and n signifies the past with respect to $n + 1$.

[0014] The present invention also relates to an atrial fibrillation detection system according to the first aspect, wherein the atrial fibrillation detection system is characterized by being provided with premature ventricular contraction exclusion means that excludes from the normalized heartbeat periods those normalized heartbeat periods that relate to premature ventricular contractions.

[0015] The present invention also relates to an atrial fibrillation detection system according to the second aspect, wherein the atrial fibrillation detection system is characterized in that the premature ventricular contraction exclusion means is configured to exclude normalized heartbeat periods that relate to premature

$$DR(N)_n = \frac{N(R_{n-1} - R_n)}{\sum_{k=n-N+1}^n R_k} \quad \dots\dots (14)$$

(N is an integer greater than 1)

[0016] Thus, for the atrial fibrillation patient, the proportion of normalized heartbeat periods that are distributed to the outside of twice the standard deviation for the healthy individual is greatest at a normalized heartbeat period of $N = 2$, and it is therefore appropriate to employ the normalized heartbeat period $DR(2)$ in order to distinguish between the healthy individual and the atrial fibrillation patient by counting abnormal normalized heartbeat periods; however, it is also possible to distinguish an atrial fibrillation patient by using an integer other than 2.

[0017] Therefore, the atrial fibrillation patient can be distinguished by employing the aforementioned equation (1).

•Method for detecting atrial fibrillation

[0018] The validity of the method of counting, from among a prescribed number of continuous normalized heartbeat periods, those having an absolute value that exceeds a prescribed normal heartbeat period threshold value, and determining atrial fibrillation to be present when the count has exceeded a prescribed normal cumulative count threshold value, will be examined.

[0019] First, as one case, a case that involves adopting the normalized heartbeat period $DR(2)$, then dividing a time series of heartbeat periods into intervals of 10 beats each, and counting the number of abnormal $DR(2)$ for which $|DR(2)| > T_N = 0.112$ that occur during these 10 beats, shall be examined. As shown in FIG. 5, for the atrial fibrillation patient, abnormal $DR(2)$ values constituted 74.6 of the total frequency, and therefore the averaged abnormal fibrillation detection

system is characterized by being provided with a premature atrial contraction exclusion means that excludes from the normalized heartbeat periods those normalized heartbeat periods that relate to premature atrial contractions.

[0020] The present invention also relates to an atrial fibrillation detection system according to the third aspect, wherein the atrial fibrillation detection system is characterized by being provided with a premature atrial contraction exclusion means that excludes from the normalized heartbeat periods those normalized heartbeat periods that relate to premature atrial contractions.

[0021] The present invention also relates to an atrial fibrillation detection system according to the fourth aspect, wherein the atrial fibrillation detection system is characterized in that the premature atrial contraction exclusion means is configured to exclude normalized heartbeat periods that relate to premature atrial contractions, by the following method.

[0022] From among the normalized heartbeat periods $DR(N)_i$ from a time series R_i of heartbeat periods of the heart, a normalized heartbeat period $DR(N)_i$ that satisfies the following equations (5) and (6) is retrieved. Then $DR(N)_i$ and the value $DR(N)_{i+1}$ successive thereto are excluded from the retrieved normalized heartbeat period $DR(N)_i$.

$$\frac{R_i + R_{i+1} - 2\bar{R}_{i-1}(M)}{2\bar{R}_{i-1}(M)} < 2T_A \quad \dots\dots (5)$$

$$\frac{(K+1)|R_{i-1} - R_{i+1}|}{K\bar{R}_{i-1}(K) + R_{i+1}} < T_N \quad \dots\dots (6)$$

T_N and T_A are prescribed threshold values that satisfy the relationships $T_N > 0$ and $-T_N \leq T_A \leq 0$, subscript i is a time series, and i signifies the past with respect to $i+1$.

M is an integer equal to 1 or greater, and K is an integer equal to 0 or greater.

$\bar{R}_i(X)$ in equations (5) and (6) is represented by the following equation (7) when X is an integer equal to 1 or greater, and by the following equation (8) when $X = 0$.

$$\bar{R}_i(X) = \frac{1}{X} \sum_{k=i-X+1}^i R_k \quad \dots\dots (7)$$

$$\bar{R}_i(0) = 0 \quad \dots\dots (8)$$

[0023] The present invention also relates to an atrial fibrillation detection system according to the fifth aspect, wherein the atrial fibrillation detection system is characterized in that the premature atrial contraction exclusion means is configured to exclude normalized heartbeat periods that relate to premature atrial contractions, by the following method.

[0024] From among the normalized heartbeat periods $DR(N)_i$ from a time series R_i of heartbeat periods of the heart, a normalized heartbeat period $DR(N)_i$ that satisfies the following equations (5) and (6) is retrieved. Then $DR(N)_i$ and the value $DR(N)_{i+1}$ successive thereto are excluded from the retrieved normalized heartbeat period $DR(N)_i$.

$$\frac{R_i + R_{i+1} - 2\bar{R}_{i-1}(M)}{2\bar{R}_{i-1}(M)} < 2T_A \quad \dots\dots (5)$$

$$\frac{(K+1)|R_{i-1} - R_{i+1}|}{K\bar{R}_{i-1}(K) + R_{i+1}} < T_N \quad \dots\dots (6)$$

T_N and T_A are prescribed threshold values that satisfy the relationships $T_N > 0$ and $-T_N \leq T_A \leq 0$, subscript i is a time series, and i signifies the past with respect to $i+1$.

M is an integer equal to 1 or greater, and K is an integer equal to 0 or greater.

$\bar{R}_i(X)$ in equations (5) and (6) is represented by the following equation (7) when X is an integer equal to 1 or greater, and by the following equation (8) when X = 0.

$$\bar{R}_i(X) = \frac{1}{X} \sum_{k=i-X+1}^i R_k \quad \dots\dots (7)$$

$$\bar{R}_i(0) = 0 \quad \dots\dots (8)$$

[0025] The present invention also relates to an atrial fibrillation detection system according to the sixth aspect, wherein the atrial fibrillation detection system is characterized in that the premature atrial contraction exclusion means is configured to exclude normalized heartbeat periods that relate to premature atrial contractions, by the following method.

[0026] From among the normalized heartbeat periods $DR(N)_i$ from a time series R_i of heartbeat periods of the heart, a normalized heartbeat period $DR(N)_i$ that satisfies the following equations (5) and (6) is retrieved. Then $DR(N)_i$ and the value $DR(N)_{i+1}$ successive thereto are excluded from the retrieved normalized heartbeat period $DR(N)_i$.

$$\frac{R_i + R_{i+1} - 2\bar{R}_{i-1}(M)}{2\bar{R}_{i-1}(M)} < 2T_A \quad \dots\dots (5)$$

$$\frac{(K+1)|R_{i-1} - R_{i+1}|}{K\bar{R}_{i-1}(K) + R_{i+1}} < T_N \quad \dots\dots (6)$$

T_N and T_A are prescribed threshold values that satisfy the relationships $T_N > 0$ and $-T_N \leq T_A \leq 0$, subscript i is a time series, and i signifies the past with respect to i + 1.

M is an integer equal to 1 or greater, and K is an integer equal to 0 or greater.

$\bar{R}_i(X)$ in equations (5) and (6) is represented by the following equation (7) when X is an integer equal to 1 or greater, and by the following equation (8) when X = 0.

$$\bar{R}_i(X) = \frac{1}{X} \sum_{k=i-X+1}^i R_k \quad \dots\dots (7)$$

$$\bar{R}_i(0) = 0 \quad \dots\dots (8)$$

[0027] The present invention also relates to an atrial fibrillation detection system according to any of the first to ninth aspects, wherein the atrial fibrillation detection system is characterized in that the normalized heartbeat period computation means is configured to compute a normalized heartbeat period $DR(2)_n$, represented by the following equation (9), from the heartbeat periods.

$$DR(2)_n = \frac{2(R_{n-1} - R_n)}{R_{n-1} + R_n} \quad \dots\dots (9)$$

[0028] The present invention also relates to an atrial fibrillation detection system according to any of the first to ninth aspects, wherein the atrial fibrillation detection system is characterized by comprising a sensor for heartbeat measurement

provided with the heartbeat period measurement means, and an analyzer provided with the normalized heartbeat period computation means, the abnormal normalized heartbeat period cumulation means, and the comparison/determination means.

[0029] The present invention also relates to an atrial fibrillation detection system according to the tenth aspect, wherein the atrial fibrillation detection system is characterized by comprising a sensor for heartbeat measurement provided with the heartbeat period measurement means, and an analyzer provided with the normalized heartbeat period computation means, the abnormal normalized heartbeat period cumulation means, and the comparison/determination means.

[0030] The present invention also relates to an atrial fibrillation detection system according to the eleventh aspect, wherein the atrial fibrillation detection system is characterized in that the sensor is provided with a heartbeat period storage means for storing heartbeat periods measured by the heartbeat period measurement means, or provided with heartbeat period transmission means for transmitting to an analyzer the measured heartbeat periods, the system being configured such that atrial fibrillation is detected by inputting the heartbeat periods measured using the sensor to the analyzer via the heartbeat period storage means or the heartbeat period transmission means.

[0031] The present invention also relates to an atrial fibrillation detection system according to the twelfth aspect, wherein the atrial fibrillation detection system is characterized in that the sensor is provided with a heartbeat period storage means for storing heartbeat periods measured by the heartbeat period measurement means, or provided with heartbeat period transmission means for transmitting to an analyzer the measured heartbeat periods, the system being configured such that atrial fibrillation is detected by inputting the heartbeat periods measured using the sensor to the analyzer via the heartbeat period storage means or the heartbeat period transmission means.

EFFECT OF THE INVENTION

[0032] The present invention, by being configured as described above, makes it possible to detect (symptoms of) atrial fibrillation using only heartbeat period values measured over a brief time period, so that the burden on the test subject can be reduced, and makes it possible to detect even paroxysmal atrial fibrillation, and moreover to accomplish this using a compact measuring device for measuring only heartbeat periods of the heart, thus making use in the home possible, and contributing to early detection of atrial fibrillation.

BRIEF DESCRIPTION OF THE DRAWINGS

[0033]

FIG. 1 is a graph showing a frequency distribution of ΔR in a healthy individual;
 FIG. 2 is a graph showing a frequency distribution of ΔR in an atrial fibrillation patient;
 FIG. 3 is a graph showing a frequency distribution of DR(1) in an atrial fibrillation patient;
 FIG. 4 is a graph showing a frequency distribution of DR(2) in a healthy individual;
 FIG. 5 is a graph showing a frequency distribution of DR(2) in an atrial fibrillation patient;
 FIG. 6 is a graph showing a distribution of abnormal DR(2) count during 10 beats in a healthy individual;
 FIG. 7 is a graph showing a distribution of abnormal DR(2) count during 10 beats in an atrial fibrillation patient;
 FIG. 8 is a graph showing a distribution of abnormal DR(2) count during 20 beats in a healthy individual;
 FIG. 9 is a graph showing a distribution of abnormal DR(2) count during 20 beats in an atrial fibrillation patient;
 FIG. 10 is a graph showing a distribution of abnormal DR(2) count during 20 beats in an individual having premature atrial contractions;
 FIG. 11 is a diagrammatic illustration of a typical premature ventricular contraction electrocardiographic complex;
 FIG. 12 is a diagrammatic illustration of a typical premature atrial contraction electrocardiographic complex;
 FIG. 13 is a graph showing a distribution of abnormal DR(2) count during 10 beats in a healthy individual, after elimination of premature ventricular contractions;
 FIG. 14 is a graph showing a distribution of abnormal DR(2) count during 20 beats in an individual having premature atrial contractions, after elimination of premature atrial contractions;
 FIG. 15 is a graph showing a distribution of abnormal DR(2) count during 20 beats in a healthy individual, after elimination of premature atrial and ventricular contractions;
 FIG. 16 is a graph showing a distribution of abnormal DR(2) count during 20 beats in an atrial fibrillation patient, after elimination of premature atrial and ventricular contractions;
 FIG. 17 is a diagrammatic illustration of configuration of the present embodiment;
 FIG. 18 is a diagrammatic illustration of configuration of the present embodiment; and
 FIG. 19 is a diagrammatic illustration of configuration of another example.

DETAILED DESCRIPTION OF THE INVENTION

[0034] The presently preferred embodiments of the present invention are described in brief below, to show the operation of the present invention on the basis of the drawings.

[0035] It has been verified that a determination of atrial fibrillation can be made in cases in which, from among a prescribed number (as discussed below, about 20 at the most) of normalized heartbeat periods $DR(N)$, those having absolute values that exceed a prescribed normal heartbeat period threshold value are counted as abnormal normalized heartbeat periods, and the count of these abnormal normalized heartbeat periods is found to exceed a prescribed normal cumulative count threshold value. It is therefore easy to detect whether or not a subject has atrial fibrillation.

[0036] Moreover, it is possible to detect symptoms of atrial fibrillation from heartbeat period values measured over a brief time period, commensurately reducing the burden on the test subject, and it is also possible to detect paroxysmal atrial fibrillation occurring within a brief time period.

[0037] Additionally, normalized heartbeat periods $DR(N)$ can be computed from the heartbeat periods of a subject, thereby obviating the need to employ a specialized device of the type normally used to detect paroxysmal atrial fibrillation, such as a Holter monitor electrocardiograph, twelve-lead resting electrocardiograph, or other such relatively bulky device for which the electrode locations are strictly specified, so that normalized heartbeat periods $DR(N)$ can be calculated from heartbeat periods measured, for example, with a heart rate meter designed to be stuck to the chest, a wristband type plethysmograph, or other compact measurement device that can easily be used at home, and by the procedure described above, it can be detected whether or not there is atrial fibrillation.

Embodiments

[0038] A specific embodiment of the present invention will be described on the basis of the drawings.

[0039] The present embodiment is an atrial fibrillation detection system 1 for detecting the presence of atrial fibrillation in a subject, provided with a heartbeat period measurement means 4 that measures heartbeat periods of the heart; a normalized heartbeat period computation means 7 that computes normalized heartbeat periods $DR(N)$, represented by the preceding equation (1), where R_n is a time series of heartbeat periods of the heart, from heartbeat periods of the heart that were measured by the heartbeat period measurement means 4; an abnormal normalized heartbeat period cumulation means 10 that adds up the count of abnormal normalized heartbeat periods having an absolute value that exceeds a normal heartbeat period value, from among a prescribed number of successive normalized heartbeat periods $DR(N)$; and a comparison/determination means 12 that compares the cumulative count of the abnormal normalized heartbeat periods and a normal cumulative count threshold value, and in the event that the cumulative count of the abnormal normalized heartbeat periods exceeds the normal cumulative count threshold value, determines that atrial fibrillation has occurred.

[0040] More specifically, as shown in FIG. 17, the present embodiment is constituted by a sensor 2 for heartbeat period measurement, which is provided with the heartbeat period measurement means 4; and an analyzer 3 which is provided with the normalized heartbeat period computation means 7, the abnormal normalized heartbeat period cumulation means 10, and the comparison/determination means 12.

[0041] Each part is described in specific terms below.

[0042] The sensor 2 is provided with the heartbeat period measurement means 4, and with a heartbeat period transmission means 5 for transmitting the heartbeat period data measured by the heartbeat period measurement means 4, to a heartbeat period reception means 6 of the analyzer 3.

[0043] The heartbeat period measurement means 4 is configured, for example, to use a microcomputer or the like to measure the heartbeat period from the interval between an R wave and another neighboring R wave, or from the interval between an S wave and another neighboring S wave, in an electrocardiogram based on changes in voltage obtained from electrodes. Consequently, where a compact sensor is stuck to the skin via electrodes, the sensor can be hidden beneath the clothing, and measurements can be performed without hampering daily activities.

[0044] Optionally, the heartbeat period measurement means 4 may be configured, for example, to measure the pulse wave from reflected infrared light, and to measure the heartbeat periods from the peak intervals thereof, or the like. In this case, it will suffice simply to fasten the sensor to the earlobe, the wrist, the arm, or the like with a clip or band, for ease of wear. Configurations in which heartbeat periods are measured by electrical processing of cardiac sound or pulse sound are also acceptable. In this case, it will be possible to house the sensor inside a stethoscope or blood pressure gauge, so as to promote widespread use.

[0045] The heartbeat period measurement means 4 transfers the measured heartbeat period data to the heartbeat period transmission means 5.

[0046] The heartbeat period transmission means 5 transfers the heartbeat period data received from the heartbeat period measurement means 4 to the heartbeat period reception means 6 which is provided to the analyzer 3. In the present embodiment, a wireless arrangement employing radio waves or light is adopted as the transfer method. In this

case, the sensor can be more compact, and the subject can measure heartbeat periods without hindering daily activities. Alternatively, a wired arrangement may be adopted as the transfer method, employing, for example, wiring on a printed circuit board, an electrical cable, or an optical cable. This is appropriate in cases of building a system in which the sensor and analyzer are integrated. It is also possible to employ phone lines, the internet, or other public communications lines, in which case it will be possible to detect atrial fibrillation of the subject remotely.

[0047] The analyzer 3 is provided with the heartbeat period reception means 6, the normalized heartbeat period computation means 7, the abnormal normalized heartbeat period cumulation means 10, a prescribed threshold value storage means 11, the comparison/determination means 12, and a display means 13. The analyzer 3 is an electronic calculator or measuring device for performing a series involving computation, comparison, and display; a dedicated device, PC, tablet computer, smartphone, mobile phone, or the like provided with each of the aforementioned means can be adopted.

[0048] The heartbeat period reception means 6 receives heartbeat period data from the heartbeat period transmission means 5 of the sensor 2, and transfers the data to the normalized heartbeat period computation means 7.

[0049] The normalized heartbeat period computation means 7 computes normalized heartbeat periods by a prescribed method, and transfers the normalized heartbeat periods to the abnormal normalized heartbeat period cumulation means 10.

[0050] The abnormal normalized heartbeat period cumulation means 10 makes reference to a normal heartbeat period threshold value, stored in the prescribed threshold value storage means 11, for recognizing abnormal normalized heartbeat periods, and from the normalized heartbeat periods in intervals containing prescribed numbers of heartbeats, takes a cumulative count of those that have an absolute value that exceeds the normal heartbeat period threshold value, designating these as abnormal normalized heartbeat periods; and then transfers the abnormal normalized heartbeat period count per prescribed heart rate interval to the comparison/determination means 12.

[0051] The comparison/determination means 12, making reference to a normal cumulative count threshold value per prescribed heart rate interval, which is stored in the prescribed threshold value storage means 11, detects any prescribed heart rate interval in which the abnormal normalized heartbeat period count for the prescribed heart rate interval exceeds the normal cumulative count threshold value, as being a point of occurrence of atrial fibrillation, and transfers the results to the display means 13.

[0052] The display means 13 displays whether or not atrial fibrillation has been detected. As the display means 13, there can be employed a display for displaying text, images, or the like. In this case, a time series of heartbeat periods can be displayed, together with the time, as a graph, to produce an easy-to-understand display indicating when the heartbeat period in which atrial fibrillation occurred was observed. Light, sound, or vibration can also be employed as the display means 13. In this case, immediate notification that atrial fibrillation has occurred can be provided. For example, an LED can be employed as light source, a buzzer or earphone as a sound source, or a motor as a vibration source.

[0053] With the aforescribed configuration (the atrial fibrillation detection system 1), it is possible to detect atrial fibrillation; however, in the present embodiment, in order to further improve the detection accuracy, a configuration like the atrial fibrillation detection system 16 depicted in FIG. 18, in which an analyzer 17 is further provided with a premature atrial contraction exclusion means 8 for excluding normalized heartbeat periods that relate to premature atrial contractions, and a premature ventricular contraction exclusion means 9 for excluding normalized heartbeat periods that relate to premature ventricular contractions, is acceptable. Detection accuracy can be improved even with configuration provided only with either the premature atrial contraction exclusion means 8 or the premature ventricular contraction exclusion means 9.

[0054] Specifically, the premature atrial contraction exclusion means 8 is configured to retrieve, from the normalized heartbeat periods $DR(N)_i$ from a time series R_i of heartbeat periods of the heart, normalized heartbeat periods $DR(N)_i$ that satisfy the preceding equations (5) and (6), and to then exclude $DR(N)_i$ and $DR(N)_{i+1}$ successive thereto from the retrieved normalized heartbeat periods $DR(N)_i$, to exclude normalized heartbeat periods that relate to premature atrial contractions.

[0055] The premature ventricular contraction exclusion means 9 is configured to retrieve, from the normalized heartbeat periods $DR(N)_i$ from a time series R_i of heartbeat periods of the heart, a normalized heartbeat period $DR(N)_i$ that satisfies the preceding equations (2) and (3), and then to exclude the $DR(N)_i$ and the two values $DR(N)_{i+1}$ and $DR(N)_{i+2}$ successive thereto from the retrieved normalized heartbeat period $DR(N)_i$, to exclude normalized heartbeat periods that relate to premature ventricular contractions.

[0056] In cases in which the premature atrial contraction exclusion means 8 and the premature ventricular contraction exclusion means 9 are provided, the process is as follows.

[0057] From among the normalized heartbeat periods that were calculated by the normalized heartbeat period computation means 7, normalized heartbeat periods that relate to premature atrial contractions are excluded in accordance with a prescribed procedure by the premature atrial contraction exclusion means 8.

[0058] In accordance with a prescribed procedure, the premature ventricular contraction exclusion means 9 excludes normalized heartbeat periods that relate to premature ventricular contractions from the normalized heartbeat periods

that were calculated by the normalized heartbeat period computation means 7.

[0059] The procedure of either the premature atrial contraction exclusion means 8 or the premature ventricular contraction exclusion means 9 may take place first. After normalized heartbeat periods that relate to premature atrial contractions and normalized heartbeat periods that relate to premature ventricular contractions have been excluded, the normalized heartbeat periods are transferred to the abnormal normalized heartbeat period computation means 10, and processed by the abnormal normalized heartbeat period computation means 10 and the comparison/determination means 12 as mentioned above.

[0060] In another acceptable configuration like that in the additional example depicted in FIG. 19 (atrial fibrillation detection system 18), a sensor 19 is provided with a heartbeat period storage means 14 in place of the heartbeat period transmission means 5 of the present embodiment, and an analyzer 20 is provided with a heartbeat period readout means 15 in place of the heartbeat period reception means 6 of the present embodiment. The heartbeat period storage means 14 of the sensor 19 stores the heartbeat periods that have been measured by the heartbeat period measurement means 4. Specifically, a tape, semiconductor memory, or the like can be adopted. Unlike a Holter monitor electrocardiograph, there is no need to store electrocardiographic complexes, and in cases in which a semiconductor memory is employed as the heartbeat period storage means 14, an extremely compact memory having low power consumption can be employed, thereby making possible a compact and lightweight configuration for the sensor 19, so as not to impose a burden on the test subject. The heartbeat period readout means 15 of the sensor 20 reads out the heartbeat periods stored in the heartbeat period storage means 14 of the sensor 19, and transfers the heartbeat periods to the normalized heartbeat period computation means 7. As to the timing for readout, readout may take place in real time while measurement is ongoing, or readout in bulk may take place after a prescribed measurement duration. The route by which the heartbeat periods are read out from the heartbeat period storage means 14 may be wired or wireless. In the case of a wired arrangement, for example, USB or RS-232C can be employed, for rapid and reliable readout of heartbeat periods. In the case of a wireless arrangement, either light or radio waves are acceptable, and heartbeat periods can be easily read out by the user, providing a more practical system.

[0061] The reason for adopting a method that employs the aforementioned equations (1) to (9) when detecting atrial fibrillation is discussed in detail below.

• ΔR distributions of healthy individuals and atrial fibrillation patients

[0062] From the heartbeat periods respectively recorded over two hours in four healthy individuals and five atrial fibrillation patients, distributions of the difference ΔR between neighboring heartbeat periods were examined. The ΔR distributions of the healthy individuals and the atrial fibrillation patients are shown respectively in FIG. 1 and FIG. 2. The horizontal axis is a scale having a scale interval of 10 ms, and the vertical axis is frequency. A simple glance suffices to appreciate that the distribution is wider for the atrial fibrillation patients than for the healthy individuals. It may be thought that atrial fibrillation can be detected when large ΔR values are counted. However, this difference in the distributions cannot simply be employed to detect atrial fibrillation. The reason is that the magnitude of fluctuation of heartbeat periods differs depending on the average heart rate, i.e., the average heartbeat period. For example, during exercise, a person's heart rate is high, i.e., the heartbeat period is small, but fluctuation of the heartbeat period at this time is small. Consequently, it is necessary to normalize ΔR by some heartbeat period value. First, the distribution of normalized heartbeat periods, defined by the following equation (10), for the atrial fibrillation patients was examined.

$$DR(1)_n = \frac{R_{n-1} - R_n}{R_{n-1}} \quad \dots\dots (10)$$

[0063] Here, R is the heartbeat period, subscript n is a time series, and n signifies the past with respect to n + 1. The distribution of $DR(1)_n$ is plotted in FIG. 3. The horizontal axis is a scale having a scale interval of 0.01, and the vertical axis is frequency. Because the distribution is asymmetrical, $DR(1)_n$ is unsuited to detecting atrial fibrillation. A case of using the definition

$$DR(1)_n = \frac{R_{n-1} - R_n}{R_n} \quad \dots\dots (11)$$

was examined as well, but as in FIG. 3, an asymmetrical result for the distribution was obtained. Next, distributions for a healthy individual and an atrial fibrillation patient obtained using normalized heartbeat periods defined by the following

equation (12) (the following equation (12) is the same as equation (9)) were examined.

$$DR(2)_n = \frac{2(R_{n-1} - R_n)}{R_{n-1} + R_n} \quad \dots\dots (12)$$

[0064] These are shown respectively in FIG. 4 and FIG. 5. The horizontal axis is a scale having a scale interval of 0.01, and the vertical axis is frequency. The standard deviation of the distribution for the healthy individuals was $\sigma = 0.0560$, and the standard deviation of the distribution for the atrial fibrillation patients was $\sigma = 0.355$. As shown in FIG. 5, in the distribution for the atrial fibrillation patients, 74.6% of actually measured total frequency for the atrial fibrillation patient were distributed outside the range of $\pm 2\sigma = \pm 0.112$, which is equal to twice the standard deviation for the healthy individual. Thus, it is conceivable that atrial fibrillation can be detected by designating a normal normalized heartbeat period T_N for the healthy individual, and counting normalized heartbeat periods that are greater than T_N among a prescribed number of beats. For example, with the normal normalized heartbeat period set to 2σ in the distribution for healthy individuals obtained previously, when the number of abnormal normalized heartbeat periods for which $|DR(2)| > T_N = 0.112$ during 10 beats is counted, it can be expected that the abnormal normalized heartbeat period count for the healthy individuals will be 0, while that for the atrial fibrillation patients will be 7 (since 74.6% of the total frequency for the atrial fibrillation patient is distributed outside the range of $\pm 2\sigma = \pm 0.112$, it is thought that 7 beats out of 10 will lie outside that range), and therefore atrial fibrillation can be distinguished by this method. In terms of increasing the accuracy of distinction, a large difference in the aforementioned distributions between the healthy individual and the atrial fibrillation patient is better. Accordingly, distributions of normalized heartbeat periods defined by the following equation (13) for the healthy individual and for the atrial fibrillation patient were examined.

$$DR(10)_n = \frac{10(R_{n-1} - R_n)}{\sum_{k=n-9}^n R_k} \quad \dots\dots (13)$$

[0065] The standard deviation of the distribution for the healthy individuals was $\sigma = 0.0590$, and the standard deviation of the distribution for the atrial fibrillation patients was $\sigma = 0.371$. In the distribution for the atrial fibrillation patient, 72.0% of the actually measured total frequency for the atrial fibrillation patient was distributed outside the range of $\pm 2\sigma = \pm 0.118$ for the healthy individual. This is smaller than the distribution obtained from $DR(2)$. The normalized heartbeat period was further generalized as in the following equation (14) (the following equation (14) is the same as equation (1)), and a case in which $N > 10$ was examined, but the trend was the same as when $N = 10$.

$$DR(N)_n = \frac{N(R_{n-1} - R_n)}{\sum_{k=n-N+1}^n R_k} \quad \dots\dots (14)$$

(N is an integer equal to 1 or greater)

[0066] Thus, for the atrial fibrillation patient, the proportion of normalized heartbeat periods that are distributed to the outside of twice the standard deviation for the healthy individual is greatest at a normalized heartbeat period of $N = 2$, and it is therefore appropriate to employ the normalized heartbeat period $DR(2)$ in order to distinguish between the healthy individual and the atrial fibrillation patient by counting abnormal normalized heartbeat periods; however, it is also possible to distinguish an atrial fibrillation patient by using an integer other than 2.

[0067] Therefore, the atrial fibrillation patient can be distinguished by employing the aforementioned equation (1).

•Method for detecting atrial fibrillation

[0068] The validity of the method of counting, from among a prescribed number of continuous normalized heartbeat periods, those having an absolute value that exceeds a prescribed normal heartbeat period threshold value, and determining atrial fibrillation to be present when the count has exceeded a prescribed normal cumulative count threshold value, will be examined.

[0069] First, as one case, a case that involves adopting the normalized heartbeat period $DR(2)$, then dividing a time

series of heartbeat periods into intervals of 10 beats each, and counting the number of abnormal DR(2) for which $|DR(2)| > T_N = 0.112$ that occur during these 10 beats, shall be examined. As shown in FIG. 5, for the atrial fibrillation patient, abnormal DR(2) values constituted 74.6 of the total frequency, and therefore the averaged abnormal DR(2) count in each interval is 7. For the healthy individual, on the other hand, abnormal DR(2) values are expected to be 4.55% of the total frequency, and therefore the count is thought to be about 0 to 1. Accordingly, taking a value between 0 and 7, it was decided to make a determination of atrial fibrillation when the abnormal DR(2) count per interval is greater than 2. The abnormal DR(2) counts in each of 10-beat intervals for the healthy individual and the atrial fibrillation patient were examined; plots of the abnormal count and frequency thereof are shown respectively in FIG. 6 and FIG. 7. The horizontal axis is the abnormal DR(2) count in each interval, and the vertical axis is the frequency. When atrial fibrillation is designated as "positive" and normal (healthy individual) as "negative," as indicated in FIG. 7, for the atrial fibrillation patient, there were eight false-negative intervals in which the abnormal DR(2) count was 2 or less from among a total of 3,906 intervals, for a false-negative proportion of 0.205%. As indicated in FIG. 6, for the healthy individual, there were 67 false-positive intervals from among a total of 3,898 intervals, for a false-positive proportion of 1.72%. The frequency of an abnormal DR(2) count of 3 was particularly high; this is attributed to premature ventricular contraction. Because isolated premature ventricular contractions frequently occur in the healthy individual as well, it is necessary to consider methods for excluding these premature contractions.

[0070] Next, an instance of adopting DR(2) as the normalized heartbeat period, dividing a time series of heartbeat periods into intervals of 20 beats each, and counting the number of abnormal DR(2) for which $|DR(2)| > T_N = 0.112$ that occur during these 20 beats was examined. At this time, the abnormal DR(2) count for the atrial fibrillation patient can be expected to be about 15, while that for the healthy individual is thought to be about 1. Accordingly, taking a value between 15 and 1, it was decided to make a determination of atrial fibrillation when the abnormal DR(2) count per interval is greater than 6. The abnormal DR(2) count in each of 20-beat intervals for the healthy individual and the atrial fibrillation patient were examined; plots of the abnormal DR(2) count and frequency thereof are shown respectively in FIG. 8 and FIG. 9. As indicated in FIG. 8, for the healthy individual, there were five false-positive intervals from among a total of 1,949 intervals, for a false-positive proportion of 0.257%. As indicated in FIG. 9, for the atrial fibrillation patient, there were two false-negative intervals from among a total of 1,953 intervals, for a false-negative proportion of 0.102%. In both instances, the proportion of false-positives and false-negatives was smaller than when a time series of heartbeat periods was evaluated by division into intervals of 10 beats each. Consequently, it is suitable to employ the abnormal DR(2) count within 20 beats, to detect atrial fibrillation (i.e., it is suitable to employ the preceding equation (9)). While it is thought that employing an even greater number of heartbeats would reduce false-positives and false-negatives, if the number is too great, the inability to detect paroxysmal atrial fibrillation occurring within a short time period becomes a concern.

•Verification in individuals having premature atrial contraction

[0071] As described above, it has been shown that a determination of atrial fibrillation can be made when, using an abnormal normalized heartbeat period of $|DR(2)| > T_N = 0.112$, the abnormal DR(2) count from among 20 beats is greater than 6. It was examined whether this method can be used to distinguish between premature atrial contraction and atrial fibrillation. A premature atrial contraction is a premature contractions that simply occurs one at a time in isolated fashion, and poses no health risk.

[0072] Heartbeat periods of an individual having premature atrial contractions was monitored over a two-hour period, to investigate the abnormal DR(2) count within each of 20-beat intervals; FIG. 10 is a plot of the abnormal DR(2) count and frequency thereof. Out of a total frequency of 426 intervals, there were false-positives in 148 intervals, for a false-positive proportion of 34.7%. Under these circumstances, atrial fibrillation and premature atrial contractions posing no threat to health cannot be distinguished, and it is therefore necessary to exclude premature atrial contractions.

•Exclusion of premature contractions

Method for excluding premature ventricular contractions

[0073] FIG. 11 shows an electrocardiographic complex of a typical premature ventricular contraction. In it, beat C corresponds to the premature ventricular contraction. Beat C appears earlier than would a beat produced at the sinus rate, and is followed by a return to the sinus rate with beat D. Therefore, the values of $|DR(2)|$ corresponding to the heartbeat periods BC, CD, and DE are large. This is why, in FIG. 6, intervals in which the abnormal DR(2) count per interval is 3 were so numerous.

[0074] As shown in FIG. 11, the heartbeat periods of a premature ventricular contraction have a relationship that can be approximated as $2 \times AB \approx BC + CD \approx 2 \times DE$, and that generally satisfies the equation $0.75 \times AB > BC$. Accordingly, in order to exclude normalized heartbeat periods that relate to premature ventricular contractions, which may take on

abnormal values, a location that corresponds to the following equations (15) and (16) is retrieved from a time series of heartbeat periods (the following equations (15) and (16) are respectively the same as equation (2) and equation (3)).

$$|DR(N)_i| > T_p \quad \dots\dots (15)$$

$$\frac{|R_i + R_{i+1} - 2\bar{R}_{i-1}(M)|}{2\bar{R}_{i-1}(M)} < 2T_N \quad \dots\dots (16)$$

[0075] Here, R is the heartbeat period, T_p and T_N are prescribed threshold values that satisfy the relationships $T_p > 0$ and $T_N > 0$, subscript i is a time series, and i signifies the past with respect to i + 1. The retrieved R_i corresponds to the heartbeat period BC in FIG. 11. When X is an integer equal to 1 or greater, $\bar{R}_i(X)$ is represented by the following equation (17) (the following equation (17) is the same as equation (4)).

$$\bar{R}_i(X) = \frac{1}{X} \sum_{k=i-X+1}^i R_k \quad \dots\dots (17)$$

M is an integer equal to 1 or greater. When the location in question has been detected, $DR(N)_i$ and the two values $DR(N)_{i+1}$ and $DR(N)_{i+2}$ successive thereto are excluded.

[0076] In view of the nature of the premature ventricular contraction, the threshold value T_p is appropriately 0.2-0.3, and more preferably 0.25. Typically, fluctuations of the heartbeat periods of a healthy individual will be within about 10%, and therefore the most appropriate threshold value T_N for identifying abnormal heartbeat periods is 0.1. While the parameter M may be any value, exclusion capability is sufficient even when $M = 1$, and considering that the amount of computation required is less than when $M > 1$, this value is the most appropriate.

[0077] Here, a case in which $T_p = 0.25$, $T_N = 0.1$, $N = 2$, and $M = 1$ will be described, taking the example of FIG. 11. Where R_i is BC, the preceding equation (15) can be written as in the following equation (18). The preceding equation (16) can be written as in the following equation (19).

$$\frac{2|AB - BC|}{AB + BC} > 0.25 \quad \dots\dots (18)$$

$$\frac{|BC + CD - 2AB|}{2AB} < 0.2 \quad \dots\dots (19)$$

[0078] To satisfy equation (18) and equation (19), the normalized heartbeat periods $DR(2)_i$, $DR(2)_{i+1}$ and $DR(2)_{i+2}$, which correspond to the heartbeat periods BC, CD, and DE, are excluded. Positing a premature ventricular contraction heartbeat period time series in which, for example, the heartbeat period values in FIG. 11 are such that $AB = DE = 1,000$ ms, $BC = 700$ ms, and $CD = 1,300$ ms, the left term of equation (18) is 0.353, and the left term of equation (19) is 0, and both equations are satisfied. The normalized heartbeat period $DR(2)_i$ which corresponds to the heartbeat period value BC at this time, when converted using equation (9), is $2(1,000-700)/(1,000+700) = 0.353$, and likewise the normalized heartbeat periods $DR(2)_{i+1}$ and $DR(2)_{i+2}$ which correspond to CD and DE are respectively -0.600 and 0.261; therefore, if $|DR(2)| > T_N$ is selected as the abnormal normalized heartbeat period, the normalized heartbeat periods $DR(2)_i$, $DR(2)_{i+1}$ and $DR(2)_{i+2}$ will be determined to be abnormal normalized heartbeat periods due to premature ventricular contraction, and must therefore be excluded.

[0079] Consequently, abnormal normalized heartbeat periods produced in the method mentioned above due to a premature ventricular contraction can be retrieved and excluded.

•Method for excluding premature atrial contractions

[0080] FIG. 12 shows an electrocardiographic complex of a typical premature atrial contraction. In it, beat C corresponds to the premature atrial contraction. Beat C appears early or irregularly, and is followed by a return to the normal sinus rate with beat D. While the premature atrial contraction is isolated, with higher frequency of occurrence, the normalized heartbeat periods corresponding to the heartbeat periods BC and CD will take on abnormal values, thereby producing a false-positive as shown in FIG. 10. As shown in FIG. 12, the heartbeat periods of the premature atrial contraction generally have a relationship such that $AB > BC$, $CD > BC$, and $AB \approx CD$. To exclude normalized heartbeat periods that relate to premature atrial contractions, which may take on abnormal values, a location that corresponds to the following equations (20) and (21) is retrieved from a time series of heartbeat periods (the following equations (20) and (21) are respectively the same as equation (5) and equation (8)).

$$\frac{R_i + R_{i+1} - 2\bar{R}_{i-1}(M)}{2\bar{R}_{i-1}(M)} < 2T_A \quad \dots\dots (20)$$

$$\frac{(K+1)|R_{i-1} - R_{i+1}|}{K\bar{R}_{i-1}(K) + R_{i+1}} < T_N \quad \dots\dots (21)$$

[0081] Here, R_i bar (X) is equation (17) (equation (17) is the same as equation (7)), and when $X = 0$, is represented by the following equation (22) (equation (22) is the same as equation (8)).

$$\bar{R}_i(0) = 0 \quad \dots\dots (22)$$

[0082] The retrieved R_i corresponds to the heartbeat period BC in FIG. 12. $T_N > 0$; T_A is a prescribed threshold value that, due to the nature of premature atrial contractions, satisfies the condition $-T_N \leq T_A \leq 0$; subscript i is a time series; and i signifies the past with respect to $i+1$. M is an integer equal to 1 or greater, and K is an integer equal to 0 or greater. When the location in question has been detected, $DR(N)_i$ and the value $DR(N)_{i+1}$ successive thereto are excluded.

[0083] As stated previously, as fluctuations of the heartbeat periods of the healthy individual are within about 10%, the most appropriate threshold value T_N is 0.1. While the exclusion capability is highest when the threshold value T_A is 0, in consideration of the fact that the beat of a premature atrial contraction appears early to an extent that exceeds fluctuations in the heartbeat period of the healthy individual, the exclusion capability is sufficient even when $T_A = T_N$. For the parameters M and K , the exclusion capability is sufficient even when $M = K = 1$, and considering that the amount of computation required is less than when $M > 1$ or $K > 1$, this value is the most appropriate.

[0084] Here, a case in which $T_N = 0.1$, $T_A = 0$, $M = K = 1$, and $N = 2$, will be described, taking the example of FIG. 12. Where R_i is BC, the preceding equation (20) can be written as in the following equation (23). The preceding equation (21) can be written as in the following equation (24).

$$BC + CD < 2AB \quad \dots\dots (23)$$

$$\frac{2|AB - CD|}{AB + CD} < 0.1 \quad \dots\dots (24)$$

[0085] To satisfy equation (23) and equation (24), the normalized heartbeat periods $DR(2)_i$ and $DR(2)_{i+1}$ which correspond to the heartbeat periods BC and CD are excluded. Positing a premature atrial contraction heartbeat period time series in which, for example, the heartbeat period values in FIG. 12 are such that $AB = CD = 1,000$ ms and $BC = 700$ ms, equation (23) is $1,700 < 2,000$, and the left term of equation (24) is 0, so both equations are satisfied. The normalized heartbeat period $DR(2)_i$ which corresponds to the heartbeat period value BC at this time, when converted using equation (9), is $2(1,000-700)/(1,000+700) = 0.353$, and likewise the normalized heartbeat period $DR(2)_{i+1}$ which corresponds to CD is 0.353; therefore, if $|DR(2)| > T_N$ is selected as the abnormal normalized heartbeat period, the normalized heartbeat periods $DR(2)_i$ and $DR(2)_{i+1}$ will be determined to be abnormal normalized heartbeat periods, due to the premature atrial

contraction, and must therefore be excluded.

[0086] Consequently, abnormal normalized heartbeat periods produced in the method mentioned above due to a premature atrial contraction can be retrieved and excluded.

•Verification of effect of excluding premature contractions

Effect of excluding premature vascular contractions

[0087] In order to confirm the effect of excluding premature vascular contractions, verification was carried out by the same method as that used to obtain FIG. 6 by employing heartbeat periods subsequent to exclusion of the premature vascular contractions. The premature vascular contraction exclusion parameter was $T_p = 0.25$, and T_N was $T_N = 0.1$. To harmonize conditions, an abnormal normalized heartbeat period of $DR(2) > 0.112$ was selected. The results are shown in FIG. 13. Of a total frequency of 3,893 intervals, 39 intervals were false-positive, for a false-positive proportion of 1.00%. This is an improvement compared to the 1.72% observed prior to exclusion of premature vascular contractions, and therefore exclusion of premature vascular contractions can be considered effective. However, this proportion is large in comparison with the false-positive rate of 0.257% obtained in the case of evaluation using 20 beats, as shown in FIG. 8. Consequently, it is considered acceptable to employ the abnormal $DR(2)$ count during 20 beats, in order to detect atrial fibrillation.

Effect of excluding premature atrial contractions

[0088] For the one individual having premature atrial contractions mentioned previously, after carrying out a process to exclude the premature atrial contractions, a time series of heartbeat periods was divided into intervals of 20 beats each, and the count of abnormal normalized heartbeat periods in each interval was examined. For this verification, a normalized heartbeat period $DR(2)$ with parameter N set to $N = 2$ was employed. T_N was set to $T_N = 0.1$. That is, the abnormal normalized heartbeat period is such that $|DR(2)| > 0.1$. The parameters of the filter needed in equation (21) and equation (22) were set to $M = K = 1$, and the threshold value T_A was set to $T_A = 0$. The abnormal $DR(2)$ count and frequency thereof for each 20-beat interval are plotted in FIG. 14. Of a total frequency of 271 intervals, 3 intervals were false-positive, for a false-positive proportion of 0.011%. This is much smaller in comparison with the proportion of 34.7% observed prior to exclusion of premature atrial contractions, and shows that the premature atrial contraction exclusion method discussed above is effective.

•Comprehensive verification including exclusion of premature contractions

[0089] Using a normalized heartbeat period $DR(2)$, after excluding premature atrial contractions and premature ventricular contractions, a time series of heartbeat periods was divided into intervals of 20 beats each, deeming atrial fibrillation to have occurred when the abnormal normalized heartbeat period exceeded 6 within this 20-beat interval. The normal normalized heartbeat period was $T_N = 0.1$, and the abnormal normalized heartbeat period was $|DR(2)| > T_N$. The premature atrial contraction exclusion parameters were $M = K = 1$, and the threshold value T_A was $T_A = 0$. The premature ventricular contraction exclusion parameter was $T_p = 0.25$.

[0090] Abnormal normalized heartbeat period distributions respectively obtained from heartbeat periods of four healthy individuals and five atrial fibrillation patients over a two-hour period are shown in FIG. 15 and FIG. 16. In FIG. 15, with the healthy individuals, 3 intervals among a total frequency of 1,949 intervals were false-positive, for a false-positive proportion of 0.154%. In FIG. 16, with the atrial fibrillation patients, 4 intervals among a total frequency of 1,300 intervals were false-negative, for a false-negative proportion of 0.308%. Therefore, the method employing the aforementioned equations (1) to (9) can be considered as satisfactory for detecting atrial fibrillation from heartbeat periods.

Claims

1. An atrial fibrillation detection system (1) for detecting the presence of atrial fibrillation in a subject, wherein the atrial fibrillation detection system (1) is provided with heartbeat period measurement means (4) that is configured to measure heartbeat periods of the heart; normalized heartbeat period computation means (7); **characterised in that** the normalized heartbeat period computation means (7) is configured to compute normalized heartbeat periods $DR(N)$ represented by the following equation (1), where R_n is a time series of heartbeat periods of the heart, from heartbeat periods of the heart that were measured by the heartbeat period measurement means (4); abnormal normalized heartbeat period cumulation means (10) that, from among a prescribed number of successive normalized heartbeat periods $DR(N)$, is configured to add up the count of abnormal normalized heartbeat periods that have an

absolute value exceeding a normal heartbeat period value; and comparison/determination means (12) that is configured to compare the cumulative count of the abnormal normalized heartbeat periods and a normal cumulative count threshold value, and in the event that the cumulative count of the abnormal normalized heartbeat periods exceeds the normal cumulative count threshold value, to determine that atrial fibrillation has occurred,

$$DR(N)_n = \frac{N(R_{n-1} - R_n)}{\sum_{k=n-N+1}^n R_k} \dots\dots (1)$$

wherein N is an integer greater than 1, subscript n is a time series, and n signifies the past with respect to n + 1.

2. The atrial fibrillation detection system (1) according to claim 1, wherein the atrial fibrillation detection system (1) is **characterized by** being provided with premature ventricular contraction exclusion means (9) that excludes from the normalized heartbeat periods those normalized heartbeat periods that relate to premature ventricular contractions.
3. The atrial fibrillation detection system (1) according to claim 2, wherein the atrial fibrillation detection system (1) is **characterized in that** the premature ventricular contraction exclusion means (9) is configured to exclude normalized heartbeat periods that relate to premature ventricular contractions, by the following method, wherein from among the normalized heartbeat periods $DR(N)_i$ from a time series R_i of heartbeat periods of the heart, a normalized heartbeat period $DR(N)_i$ that satisfies the following equations (2) and (3) is retrieved, then $DR(N)_i$ and two values $DR(N)_{i+1}$ and $DR(N)_{i+2}$ successive thereto are excluded from the retrieved normalized heartbeat period $DR(N)_i$,

$$|DR(N)_i| > T_p \dots\dots (2)$$

$$\frac{|R_i + R_{i+1} - 2\bar{R}_{i-1}(M)|}{2\bar{R}_{i-1}(M)} < 2T_N \dots\dots (3)$$

wherein T_p and T_N are prescribed threshold values that satisfy the relationships $T_p > 0$ and $T_N > 0$, subscript i is a time series, and i signifies the past with respect to i + 1,
 $\bar{R}_i$ bar (X) in equation (3) is represented by the following equation (4),

$$\bar{R}_i(X) = \frac{1}{X} \sum_{k=i-X+1}^i R_k \dots\dots (4)$$

wherein M and X are integers equal to 1 or greater.

4. The atrial fibrillation detection system (1) according to claim 1, wherein the atrial fibrillation detection (1) system is **characterized by** being provided with a premature atrial contraction exclusion means (8) that excludes from the normalized heartbeat periods those normalized heartbeat periods that relate to premature atrial contractions.
5. The atrial fibrillation detection system (1) according to claim 2, wherein the atrial fibrillation detection system (1) is **characterized by** being provided with a premature atrial contraction exclusion means (8) that excludes from the normalized heartbeat periods those normalized heartbeat periods that relate to premature atrial contractions.
6. The atrial fibrillation detection system (1) according to claim 3, wherein the atrial fibrillation detection system (1) is **characterized by** being provided with a premature atrial contraction exclusion means (8) that excludes from the normalized heartbeat periods those normalized heartbeat periods that relate to premature atrial contractions.

7. The atrial fibrillation detection system (1) according to claim 4, wherein the atrial fibrillation detection system (1) is **characterized in that** the premature atrial contraction exclusion means (8) is configured to exclude normalized heartbeat periods that relate to premature atrial contractions, by the following method, wherein from among the normalized heartbeat periods $DR(N)_i$ from a time series R_i of heartbeat periods of the heart, a normalized heartbeat period $DR(N)_i$ that satisfies the following equations (5) and (6) is retrieved. Then $DR(N)_i$ and the value $DR(N)_{i+1}$ successive thereto are excluded from the retrieved normalized heartbeat period $DR(N)_i$,

$$\frac{R_i + R_{i+1} - 2\bar{R}_{i-1}(M)}{2\bar{R}_{i-1}(M)} < 2T_A \quad \dots\dots (5)$$

$$\frac{(K+1)|R_{i-1} - R_{i+1}|}{K\bar{R}_{i-1}(K) + R_{i+1}} < T_N \quad \dots\dots (6)$$

wherein T_N and T_A are prescribed threshold values that satisfy the relationships $T_N > 0$ and $-T_N \leq T_A \leq 0$, subscript i is a time series, and i signifies the past with respect to $i+1$, M is an integer equal to 1 or greater, and K is an integer equal to 0 or greater, and R_i bar (X) in equations (5) and (6) is represented by the following equation (7) when X is an integer equal to 1 or greater, and by the following equation (8) when $X = 0$,

$$\bar{R}_i(X) = \frac{1}{X} \sum_{k=i-X+1}^i R_k \quad \dots\dots (7)$$

$$\bar{R}_i(0) = 0 \quad \dots\dots (8)$$

8. The atrial fibrillation detection system (1) according to claim 5, wherein the atrial fibrillation detection system (1) is **characterized in that** the premature atrial contraction exclusion means (8) is configured to exclude normalized heartbeat periods that relate to premature atrial contractions, by the following method, wherein from among the normalized heartbeat periods $DR(N)_i$ from a time series R_i of heartbeat periods of the heart, a normalized heartbeat period $DR(N)_i$ that satisfies the following equations (5) and (6) is retrieved, and then $DR(N)_i$ and the value $DR(N)_{i+1}$ successive thereto are excluded from the retrieved normalized heartbeat period $DR(N)_i$,

$$\frac{R_i + R_{i+1} - 2\bar{R}_{i-1}(M)}{2\bar{R}_{i-1}(M)} < 2T_A \quad \dots\dots (5)$$

$$\frac{(K+1)|R_{i-1} - R_{i+1}|}{K\bar{R}_{i-1}(K) + R_{i+1}} < T_N \quad \dots\dots (6)$$

wherein T_N and T_A are prescribed threshold values that satisfy the relationships $T_N > 0$ and $-T_N \leq T_A \leq 0$, subscript i is a time series, and i signifies the past with respect to $i+1$, M is an integer equal to 1 or greater, and K is an integer equal to 0 or greater, and R_i bar (X) in equations (5) and (6) is represented by the following equation (7) when X is an integer equal to 1 or greater, and by the following equation (8) when $X = 0$,

$$\bar{R}_i(X) = \frac{1}{X} \sum_{k=i-X+1}^i R_k \quad \dots\dots (7)$$

$$\bar{R}_i(0) = 0 \quad \dots\dots (8)$$

9. The atrial fibrillation detection system (1) according to claim 6, wherein the atrial fibrillation detection system (1) is **characterized in that** the premature atrial contraction exclusion means (8) is configured to exclude normalized heartbeat periods that relate to premature atrial contractions, by the following method, wherein from among the normalized heartbeat periods $DR(N)_i$ from a time series R_i of heartbeat periods of the heart, a normalized heartbeat period $DR(N)_i$ that satisfies the following equations (5) and (6) is retrieved, and then $DR(N)_i$ and the value $DR(N)_{i+1}$ successive thereto are excluded from the retrieved normalized heartbeat period $DR(N)_i$,

$$\frac{R_i + R_{i+1} - 2\bar{R}_{i-1}(M)}{2\bar{R}_{i-1}(M)} < 2T_A \quad \dots\dots (5)$$

$$\frac{(K+1)|R_{i-1} - R_{i+1}|}{K\bar{R}_{i-1}(K) + R_{i+1}} < T_N \quad \dots\dots (6)$$

wherein T_N and T_A are prescribed threshold values that satisfy the relationships $T_N > 0$ and $-T_N \leq T_A \leq 0$, subscript i is a time series, and i signifies the past with respect to $i+1$, M is an integer equal to 1 or greater, and K is an integer equal to 0 or greater, and $\bar{R}_i(X)$ in equations (5) and (6) is represented by the following equation (7) when X is an integer equal to 1 or greater, and by the following equation (8) when $X = 0$,

$$\bar{R}_i(X) = \frac{1}{X} \sum_{k=i-X+1}^i R_k \quad \dots\dots (7)$$

$$\bar{R}_i(0) = 0 \quad \dots\dots (8)$$

10. The atrial fibrillation detection system (1) according to any of claims 1 to 9, wherein the atrial fibrillation detection system (8) is **characterized in that** the normalized heartbeat period computation means is configured to compute a normalized heartbeat period $DR(2)_n$, represented by the following equation (9), from the heartbeat periods,

$$DR(2)_n = \frac{2(R_{n-1} - R_n)}{R_{n-1} + R_n} \quad \dots\dots (9)$$

11. The atrial fibrillation detection system (1) according to any of claims 1 to 9, wherein the atrial fibrillation detection system (8) is **characterized by** comprising a sensor (19) for heartbeat measurement provided with the heartbeat period measurement means (4), and an analyzer provided with the normalized heartbeat period computation means (7), the abnormal normalized heartbeat period cumulation means (10), and the comparison/determination means.

12. The atrial fibrillation detection system (1) according to claim 10, wherein the atrial fibrillation detection system (1) is **characterized by** comprising a sensor (19) for heartbeat measurement provided with the heartbeat period meas-

urement means (4), and an analyzer provided with the normalized heartbeat period computation means (7), the abnormal normalized heartbeat period cumulation means (10), and the comparison/determination means (12).

13. The atrial fibrillation detection system (1) according to claim 11, wherein the atrial fibrillation detection system (1) is **characterized in that** the sensor (19) is provided with a heartbeat period storage means (14) for storing heartbeat periods measured by the heartbeat period measurement means (4), or provided with heartbeat period transmission means (5) for transmitting to an analyzer the measured heartbeat periods, the system (1) being configured such that atrial fibrillation is detected by inputting the heartbeat periods measured using the sensor (19) to the analyzer via the heartbeat period storage means (14) or the heartbeat period transmission means (5).
14. The atrial fibrillation detection system (1) according to claim 12, wherein the atrial fibrillation detection system (1) is **characterized in that** the sensor (19) is provided with a heartbeat period storage means (14) for storing heartbeat periods measured by the heartbeat period measurement means (4), or provided with heartbeat period transmission means (5) for transmitting to an analyzer the measured heartbeat periods, the system (1) being configured such that atrial fibrillation is detected by inputting the heartbeat periods measured using the sensor (19) to the analyzer via the heartbeat period storage means (14) or the heartbeat period transmission means (5).

Patentansprüche

1. Erkennungssystem für Vorhofflimmern (1) zum Erkennen des Vorhandenseins eines Vorhofflimmerns in einem Subjekt, wobei das Erkennungssystem für Vorhofflimmern (1) mit einem Mittel zum Messen von Herzschlagperioden (4) bereitgestellt ist, das konfiguriert ist, um Herzschlagperioden des Herzens zu messen; einem Mittel zum Berechnen normalisierter Herzschlagperioden (7); **dadurch gekennzeichnet, dass** das Mittel zum Berechnen normalisierter Herzschlagperioden (7) konfiguriert ist, um normalisierte Herzschlagperioden $DR(N)$ zu berechnen, die durch die folgende Gleichung (1) dargestellt sind, wo R_n eine Zeitreihe von Herzschlagperioden des Herzens ist, aus Herzschlagperioden des Herzens, die durch das Mittel zum Messen von Herzschlagperioden (4) gemessen wurden; einem Mittel zum Kumulieren abnormaler normalisierter Herzschlagperioden (10), das konfiguriert ist, um aus einer vorgeschriebenen Zahl aufeinanderfolgender normalisierter Herzschlagperioden $DR(N)$ die Anzahl abnormaler normalisierter Herzschlagperioden zusammenzuzählen, die einen Absolutwert aufweisen, der einen Wert normaler Herzschlagperioden überschreitet; und einem Vergleichs-/Bestimmungsmittel (12), das konfiguriert ist, um die kumulative Anzahl der abnormalen normalisierten Herzschlagperioden und einen Schwellenwert einer normalen kumulativen Anzahl zu vergleichen, und im Falle, dass die kumulative Anzahl der abnormalen normalisierten Herzschlagperioden den Schwellenwert der normalen kumulativen Anzahl überschreitet, zu bestimmen, dass Vorhofflimmern aufgetreten ist,

$$DR(N)_n = \frac{N(R_{n-1} - R_n)}{\sum_{k=n-N+1}^n R_k} \quad \dots\dots (1)$$

wobei N eine ganze Zahl größer als 1 ist, tiefgestelltes n eine Zeitreihe ist und n die Vergangenheit in Bezug auf $n + 1$ bezeichnet.

2. Erkennungssystem für Vorhofflimmern (1) nach Anspruch 1, wobei das Erkennungssystem für Vorhofflimmern (1) **dadurch gekennzeichnet ist, dass** es mit einem Mittel zum Ausschließen vorzeitiger ventrikulärer Kontraktionen (9) bereitgestellt ist, das aus den normalisierten Herzschlagperioden diejenigen normalisierten Herzschlagperioden ausschließt, die vorzeitigen ventrikulären Kontraktionen zugeordnet sind.
3. Erkennungssystem für Vorhofflimmern (1) nach Anspruch 2, wobei das Erkennungssystem für Vorhofflimmern (1) **dadurch gekennzeichnet ist, dass** das Mittel zum Ausschließen vorzeitiger ventrikulärer Kontraktionen (9) konfiguriert ist, um normalisierte Herzschlagperioden, die vorzeitigen ventrikulären Kontraktionen zugeordnet sind, durch das folgende Verfahren auszuschließen, wobei aus den normalisierten Herzschlagperioden $DR(N)_i$ aus einer Zeitreihe R_i von Herzschlagperioden des Herzens eine normalisierte Herzschlagperiode $DR(N)_i$, die die folgenden Gleichungen (2) und (3) erfüllt, gewonnen wird, dann $DR(N)_i$ und zwei darauf folgende Werte $DR(N)_{i+1}$ und $DR(N)_{i+2}$ aus der gewonnenen normalisierten Herzschlagperiode $DR(N)_i$ ausgeschlossen werden,

$$|DR(N)_i| > T_p \quad \dots\dots (2)$$

$$\frac{|R_i + R_{i+1} - 2\bar{R}_{i-1}(M)|}{2\bar{R}_{i-1}(M)} < 2T_N \quad \dots\dots (3)$$

wobei T_p und T_N vorgeschriebene Schwellenwerte sind, die die Beziehungen $T_p > 0$ und $T_N > 0$ erfüllen, tiefgestelltes i eine Zeitreihe ist und i die Vergangenheit in Bezug auf $i + 1$ bezeichnet, R_i Strich (X) in Gleichung (3) durch die folgende Gleichung (4) dargestellt ist,

$$\bar{R}_i(X) = \frac{1}{X} \sum_{k=i-X+1}^i R_k \quad \dots\dots (4)$$

wobei M und X ganze Zahlen gleich 1 oder größer sind.

4. Erkennungssystem für Vorhofflimmern (1) nach Anspruch 1, wobei das Erkennungssystem für Vorhofflimmern (1) **dadurch gekennzeichnet ist, dass** es mit einem Mittel zum Ausschließen vorzeitiger Vorhofkontraktionen (8) bereitgestellt ist, das aus den normalisierten Herzschlagperioden diejenigen normalisierten Herzschlagperioden ausschließt, die vorzeitigen Vorhofkontraktionen zugeordnet sind.
5. Erkennungssystem für Vorhofflimmern (1) nach Anspruch 2, wobei das Erkennungssystem für Vorhofflimmern (1) **dadurch gekennzeichnet ist, dass** es mit einem Mittel zum Ausschließen vorzeitiger Vorhofkontraktionen (8) bereitgestellt ist, das aus den normalisierten Herzschlagperioden diejenigen normalisierten Herzschlagperioden ausschließt, die vorzeitigen Vorhofkontraktionen zugeordnet sind.
6. Erkennungssystem für Vorhofflimmern (1) nach Anspruch 3, wobei das Erkennungssystem für Vorhofflimmern (1) **dadurch gekennzeichnet ist, dass** es mit einem Mittel zum Ausschließen vorzeitiger Vorhofkontraktionen (8) bereitgestellt ist, das aus den normalisierten Herzschlagperioden diejenigen normalisierten Herzschlagperioden ausschließt, die vorzeitigen Vorhofkontraktionen zugeordnet sind.
7. Erkennungssystem für Vorhofflimmern (1) nach Anspruch 4, wobei das Erkennungssystem für Vorhofflimmern (1) **dadurch gekennzeichnet ist, dass** das Mittel zum Ausschließen vorzeitiger Vorhofkontraktionen (8) konfiguriert ist, um normalisierte Herzschlagperioden, die vorzeitigen Vorhofkontraktionen zugeordnet sind, durch das folgende Verfahren auszuschließen,
wobei aus den normalisierten Herzschlagperioden $DR(N)_i$ aus einer Zeitreihe R_i von Herzschlagperioden des Herzens eine normalisierte Herzschlagperiode $DR(N)_i$, die die folgenden Gleichungen (5) und (6) erfüllt, gewonnen wird. Dann werden $DR(N)_i$ und der darauffolgende Wert $DR(N)_{i+1}$ aus der gewonnenen normalisierten Herzschlagperiode $DR(N)_i$ ausgeschlossen,

$$\frac{R_i + R_{i+1} - 2\bar{R}_{i-1}(M)}{2\bar{R}_{i-1}(M)} < 2T_A \quad \dots\dots (5)$$

$$\frac{(K+1)|R_{i-1} - R_{i+1}|}{K\bar{R}_{i-1}(K) + R_{i+1}} < T_N \quad \dots\dots (6)$$

wobei T_N und T_A vorgeschriebene Schwellenwerte sind, die die Beziehungen $T_N > 0$ und $-T_N \leq T_A \leq 0$ erfüllen, tiefgestelltes i eine Zeitreihe ist und i die Vergangenheit in Bezug auf $i + 1$ bezeichnet, M eine ganze Zahl gleich 1 oder größer ist, und K eine ganze Zahl gleich 0 oder größer ist, und

R_i Strich (X) in Gleichungen (5) und (6) durch die folgende Gleichung (7) dargestellt ist, wenn X eine ganze Zahl gleich 1 oder größer ist, und durch die folgende Gleichung (8), wenn X = 0 ist,

$$\bar{R}_i(X) = \frac{1}{X} \sum_{k=i-X+1}^i R_k \quad \dots\dots (7)$$

$$\bar{R}_i(0) = 0 \quad \dots\dots (8)$$

8. Erkennungssystem für Vorhofflimmern (1) nach Anspruch 5, wobei das Erkennungssystem für Vorhofflimmern (1) **dadurch gekennzeichnet ist, dass** das Mittel zum Ausschließen vorzeitiger Vorhofkontraktionen (8) konfiguriert ist, um normalisierte Herzschlagperioden, die vorzeitigen Vorhofkontraktionen zugeordnet sind, durch das folgende Verfahren auszuschließen,

wobei aus den normalisierten Herzschlagperioden $DR(N)_i$ aus einer Zeitreihe R_i von Herzschlagperioden des Herzens eine normalisierte Herzschlagperiode $DR(N)_i$, die die folgenden Gleichungen (5) und (6) erfüllt, gewonnen wird, und dann $DR(N)_i$ und der darauffolgende Wert $DR(N)_{i+1}$ aus der gewonnenen normalisierten Herzschlagperiode $DR(N)_i$ ausgeschlossen werden,

$$\frac{R_i + R_{i+1} - 2\bar{R}_{i-1}(M)}{2\bar{R}_{i-1}(M)} < 2T_A \quad \dots\dots (5)$$

$$\frac{(K+1)|R_{i-1} - R_{i+1}|}{K\bar{R}_{i-1}(K) + R_{i+1}} < T_N \quad \dots\dots (6)$$

wobei T_N und T_A vorgeschriebene Schwellenwerte sind, die die Beziehungen $T_N > 0$ und $-T_N \leq T_A \leq 0$ erfüllen, tiefgestelltes i eine Zeitreihe ist und i die Vergangenheit in Bezug auf i + 1 bezeichnet,

M eine ganze Zahl gleich 1 oder größer ist, und K eine ganze Zahl gleich 0 oder größer ist, und

R_i Strich (X) in Gleichungen (5) und (6) durch die folgende Gleichung (7) dargestellt ist, wenn X eine ganze Zahl gleich 1 oder größer ist, und durch die folgende Gleichung (8), wenn X = 0 ist,

$$\bar{R}_i(X) = \frac{1}{X} \sum_{k=i-X+1}^i R_k \quad \dots\dots (7)$$

$$\bar{R}_i(0) = 0 \quad \dots\dots (8)$$

9. Erkennungssystem für Vorhofflimmern (1) nach Anspruch 6, wobei das Erkennungssystem für Vorhofflimmern (1) **dadurch gekennzeichnet ist, dass** das Mittel zum Ausschließen vorzeitiger Vorhofkontraktionen (8) konfiguriert ist, um normalisierte Herzschlagperioden, die vorzeitigen Vorhofkontraktionen zugeordnet sind, durch das folgende Verfahren auszuschließen,

wobei aus den normalisierten Herzschlagperioden $DR(N)_i$ aus einer Zeitreihe R_i von Herzschlagperioden des Herzens eine normalisierte Herzschlagperiode $DR(N)_i$, die die folgenden Gleichungen (5) und (6) erfüllt, gewonnen wird, und dann $DR(N)_i$ und der darauffolgende Wert $DR(N)_{i+1}$ aus der gewonnenen normalisierten Herzschlagperiode $DR(N)_i$ ausgeschlossen werden,

$$\frac{R_i + R_{i+1} - 2\bar{R}_{i-1}(M)}{2\bar{R}_{i-1}(M)} < 2T_A \quad \dots\dots (5)$$

$$\frac{(K+1)|R_{i-1} - R_{i+1}|}{K\bar{R}_{i-1}(K) + R_{i+1}} < T_N \quad \dots\dots (6)$$

wobei T_N und T_A vorgeschriebene Schwellenwerte sind, die die Beziehungen $T_N > 0$ und $-T_N \leq T_A \leq 0$ erfüllen, tiefgestelltes i eine Zeitreihe ist und i die Vergangenheit in Bezug auf $i+1$ bezeichnet, M eine ganze Zahl gleich 1 oder größer ist, und K eine ganze Zahl gleich 0 oder größer ist, und R_i Strich (X) in Gleichungen (5) und (6) durch die folgende Gleichung (7) dargestellt ist, wenn X eine ganze Zahl gleich 1 oder größer ist, und durch die folgende Gleichung (8), wenn $X = 0$ ist,

$$\bar{R}_i(X) = \frac{1}{X} \sum_{k=i-X+1}^i R_k \quad \dots\dots (7)$$

$$\bar{R}_i(0) = 0 \quad \dots\dots (8)$$

10. Erkennungssystem für Vorhofflimmern (1) nach einem der Ansprüche 1 bis 9, wobei das Erkennungssystem für Vorhofflimmern (1) **dadurch gekennzeichnet ist, dass** das Mittel zum Berechnen normalisierter Herzschlagperioden konfiguriert ist, um aus den Herzschlagperioden eine normalisierte Herzschlagperiode $DR(2)_n$ zu berechnen, die durch die folgende Gleichung (9) dargestellt ist,

$$DR(2)_n = \frac{2(R_{n-1} - R_n)}{R_{n-1} + R_n} \quad \dots\dots (9)$$

11. Erkennungssystem für Vorhofflimmern (1) nach einem der Ansprüche 1 bis 9, wobei das Erkennungssystem für Vorhofflimmern (8) **dadurch gekennzeichnet ist, dass** es einen Sensor (19) zum Messen von Herzschlägen, der mit dem Mittel zum Messen von Herzschlagperioden (4) bereitgestellt ist, und einen Analysator umfasst, der mit dem Mittel zum Berechnen normalisierter Herzschlagperioden (7), dem Mittel zum Kumulieren abnormaler normalisierter Herzschlagperioden (10) und dem Vergleichs-/Bestimmungsmittel bereitgestellt ist.

12. Erkennungssystem für Vorhofflimmern (1) nach Anspruch 10, wobei das Erkennungssystem für Vorhofflimmern (1) **dadurch gekennzeichnet ist, dass** es einen Sensor (19) zum Messen von Herzschlägen, der mit dem Mittel zum Messen von Herzschlagperioden (4) bereitgestellt ist, und einen Analysator umfasst, der mit dem Mittel zum Berechnen normalisierter Herzschlagperioden (7), dem Mittel zum Kumulieren abnormaler normalisierter Herzschlagperioden (10) und dem Vergleichs-/Bestimmungsmittel (12) bereitgestellt ist.

13. Erkennungssystem für Vorhofflimmern (1) nach Anspruch 11, wobei das Erkennungssystem für Vorhofflimmern (1) **dadurch gekennzeichnet ist, dass** der Sensor (19) mit einem Mittel zum Speichern von Herzschlagperioden (14) bereitgestellt ist, um Herzschlagperioden, die durch das Mittel zum Messen von Herzschlagperioden (4) gemessen wurden, zu speichern, oder mit einem Mittel zum Übertragen von Herzschlagperioden (5) bereitgestellt ist, um die gemessenen Herzschlagperioden an einen Analysator zu übertragen, wobei das System (1) konfiguriert ist, sodass Vorhofflimmern durch Eingabe von unter Verwendung des Sensors (19) gemessenen Herzschlagperioden an den Analysator über das Mittel zum Speichern von Herzschlagperioden (14) oder das Mittel zum Übertragen von Herzschlagperioden (5) erkannt wird.

14. Erkennungssystem für Vorhofflimmern (1) nach Anspruch 12, wobei das Erkennungssystem für Vorhofflimmern (1) **dadurch gekennzeichnet ist, dass** der Sensor (19) mit einem Mittel zum Speichern von Herzschlagperioden (14) bereitgestellt ist, um Herzschlagperioden, die durch das Mittel zum Messen von Herzschlagperioden (4) gemessen wurden, zu speichern, oder mit einem Mittel zum Übertragen von Herzschlagperioden (5) bereitgestellt ist, um die gemessenen Herzschlagperioden an einen Analysator zu übertragen, wobei das System (1) konfiguriert ist, sodass Vorhofflimmern durch Eingabe von unter Verwendung des Sensors (19) gemessenen Herzschlagperioden an den Analysator über das Mittel zum Speichern von Herzschlagperioden (14) oder das Mittel zum Übertragen von Herz-

schlagperioden (5) erkannt wird.

Revendications

1. Système de détection de fibrillation auriculaire (1) pour détecter la présence d'une fibrillation auriculaire chez un sujet, dans lequel le système de détection de fibrillation auriculaire (1) est pourvu d'un moyen de mesure de périodes de battement cardiaque (4) qui est configuré pour mesurer des périodes de battement cardiaque du coeur; d'un moyen de calcul de périodes de battement cardiaque normalisées (7) ; **caractérisé en ce que** le moyen de calcul de périodes de battement cardiaque normalisées (7) est configuré pour calculer des périodes de battement cardiaque normalisées DR (N) représentées par l'équation (1) suivante, où R_n est une série chronologique de périodes de battement cardiaque du coeur, à partir de périodes de battement cardiaque du coeur qui ont été mesurées par le moyen de mesure de périodes de battement cardiaque (4) ; d'un moyen de cumul de périodes de battement cardiaque normalisées anormales (10) qui, parmi un nombre déterminé de périodes de battement cardiaque normalisées successives DR (N), est configuré pour cumuler le comptage de périodes de battement cardiaque normalisées anormales qui ont une valeur absolue dépassant une valeur de périodes de battement cardiaque normales ; et d'un moyen de comparaison/détermination (12) qui est configuré pour comparer le comptage cumulé des périodes de battement cardiaque normalisées anormales et une valeur de seuil de comptage cumulé normal, et dans le cas où le comptage cumulé des périodes de battement cardiaque normalisées anormales dépasse la valeur de seuil de comptage cumulé normal, pour déterminer qu'une fibrillation auriculaire s'est produite,

$$DR(N)_n = \frac{N(R_{n-1} - R_n)}{\sum_{k=n-N+1}^n R_k} \dots\dots (1)$$

dans lequel N est un entier supérieur à 1, l'indice n est une série chronologique, et n signifie le passé par rapport à n + 1.

2. Système de détection de fibrillation auriculaire (1) selon la revendication 1, dans lequel le système de détection de fibrillation auriculaire (1) est **caractérisé en ce qu'il** est pourvu d'un moyen d'exclusion de contractions ventriculaires prématurées (9) qui exclut des périodes de battement cardiaque normalisées les périodes de battement cardiaque normalisées qui sont relatives à des contractions ventriculaires prématurées.
3. Système de détection de fibrillation auriculaire (1) selon la revendication 2, dans lequel le système de détection de fibrillation auriculaire (1) est **caractérisé en ce que** le moyen d'exclusion de contractions ventriculaires prématurées (9) est configuré pour exclure des périodes de battement cardiaque normalisées qui sont relatives à des contractions ventriculaires prématurées, au moyen du procédé suivant,
- dans lequel parmi les périodes de battement cardiaque normalisées DR (N)_i issues d'une série chronologique R_i de périodes de battement cardiaque du coeur, une période de battement cardiaque normalisée DR (N)_i qui satisfait les équations (2) et (3) suivantes est récupérée, alors DR (N)_i et deux valeurs DR (N)_{i+1} et DR (N)_{i+2} qui la suivent sont exclues de la période de battement cardiaque normalisée DR (N)_i récupérée,

$$|DR(N)_i| > T_p \dots\dots (2)$$

$$\frac{|R_i + R_{i+1} - 2\bar{R}_{i-1}(M)|}{2\bar{R}_{i-1}(M)} < 2T_N \dots\dots (3)$$

dans lequel T_p et T_N sont des valeurs de seuil prédéterminées qui satisfont les relations $T_p > 0$ et $T_N > 0$, l'indice i est une série chronologique, et i signifie le passé par rapport à i + 1,

$\bar{R}_i$ dans l'équation (3) est représenté par l'équation (4) suivante,

$$\bar{R}_i(X) = \frac{1}{X} \sum_{k=i-X+1}^i R_k \quad \dots\dots (4)$$

dans lequel M et X sont des entiers supérieurs ou égaux à 1.

4. Système de détection de fibrillation auriculaire (1) selon la revendication 1, dans lequel le système de détection de fibrillation auriculaire (1) est **caractérisé en ce qu'il** est pourvu d'un moyen d'exclusion de contractions auriculaires prématurées (8) qui exclut des périodes de battement cardiaque normalisées les périodes de battement cardiaque normalisées qui sont relatives à des contractions auriculaires prématurées.
5. Système de détection de fibrillation auriculaire (1) selon la revendication 2, dans lequel le système de détection de fibrillation auriculaire (1) est **caractérisé en ce qu'il** est pourvu d'un moyen d'exclusion de contractions auriculaires prématurées (8) qui exclut des périodes de battement cardiaque normalisées les périodes de battement cardiaque normalisées qui sont relatives à des contractions auriculaires prématurées.
6. Système de détection de fibrillation auriculaire (1) selon la revendication 3, dans lequel le système de détection de fibrillation auriculaire (1) est **caractérisé en ce qu'il** est pourvu d'un moyen d'exclusion de contractions auriculaires prématurées (8) qui exclut des périodes de battement cardiaque normalisées les périodes de battement cardiaque normalisées qui sont relatives à des contractions auriculaires prématurées.
7. Système de détection de fibrillation auriculaire (1) selon la revendication 4, dans lequel le système de détection de fibrillation auriculaire (1) est **caractérisé en ce que** le moyen d'exclusion de contractions auriculaires prématurées (8) est configuré pour exclure des périodes de battement cardiaque normalisées qui sont relatives à des contractions auriculaires prématurées au moyen du procédé suivant,
dans lequel parmi les périodes de battement cardiaque normalisées DR (N)_i issues d'une série chronologique Ri de périodes de battement cardiaque du coeur, une période de battement cardiaque normalisée DR (N)_i qui satisfait les équations (5) et (6) suivantes est récupérée, et alors DR (N)_i et la valeur DR (N)_{i+1} qui la suit sont exclues de la période de battement cardiaque normalisée DR (N)_i récupérée,

$$\frac{R_i + R_{i+1} - 2\bar{R}_{i-1}(M)}{2\bar{R}_{i-1}(M)} < 2T_A \quad \dots\dots (5)$$

$$\frac{(K+1)|R_{i-1} - R_{i+1}|}{K\bar{R}_{i-1}(K) + R_{i+1}} < T_N \quad \dots\dots (6)$$

dans lequel T_N et T_A sont des valeurs de seuil déterminées qui satisfont les relations T_N > 0 et -T_N ≤ T_A ≤ 0, l'indice i est une série chronologique, et i signifie le passé par rapport à i + 1, M est un entier supérieur ou égal à 1, et K est un entier supérieur ou égal à 0, et R_i bar (X) dans les équations (5) et (6) est représenté par l'équation (7) suivante lorsque X est un entier supérieur ou égal à 1, et par l'équation (8) suivante lorsque X = 0,

$$\bar{R}_i(X) = \frac{1}{X} \sum_{k=i-X+1}^i R_k \quad \dots\dots (7)$$

$$\bar{R}_i(0) = 0 \quad \dots\dots (8)$$

8. Système de détection de fibrillation auriculaire (1) selon la revendication 5, dans lequel le système de détection de fibrillation auriculaire (1) est **caractérisé en ce que** le moyen d'exclusion de contractions auriculaires prématurées (8) est configuré pour exclure des périodes de battement cardiaque normalisées qui sont relatives à des contractions auriculaires prématurées au moyen du procédé suivant,

dans lequel parmi les périodes de battement cardiaque normalisées $DR(N)_i$ issues d'une série chronologique R_i de périodes de battement cardiaque du coeur, une période de battement cardiaque normalisée $DR(N)_i$ qui satisfait les équations (5) et (6) suivantes est récupérée, et alors $DR(N)_i$ et la valeur $DR(N)_{i+1}$ qui la suit sont exclues de la période de battement cardiaque normalisée $DR(N)_i$ récupérée,

$$\frac{R_i + R_{i+1} - 2\bar{R}_{i-1}(M)}{2\bar{R}_{i-1}(M)} < 2T_A \quad \dots\dots (5)$$

$$\frac{(K+1)|R_{i-1} - R_{i+1}|}{K\bar{R}_{i-1}(K) + R_{i+1}} < T_N \quad \dots\dots (6)$$

dans lequel T_N et T_A sont des valeurs de seuil déterminées qui satisfont les relations $T_N > 0$ et $-T_N \leq T_A \leq 0$, l'indice i est une série chronologique, et i signifie le passé par rapport à $i+1$, M est un entier supérieur ou égal à 1, et K est un entier supérieur ou égal à 0, et $\bar{R}_i(X)$ dans les équations (5) et (6) est représenté par l'équation (7) suivante lorsque X est un entier supérieur ou égal à 1, et par l'équation (8) suivante lorsque $X = 0$,

$$\bar{R}_i(X) = \frac{1}{X} \sum_{k=i-X+1}^i R_k \quad \dots\dots (7)$$

$$\bar{R}_i(0) = 0 \quad \dots\dots (8)$$

9. Système de détection de fibrillation auriculaire (1) selon la revendication 6, dans lequel le système de détection de fibrillation auriculaire (1) est **caractérisé en ce que** le moyen d'exclusion de contractions auriculaires prématurées (8) est configuré pour exclure des périodes de battement cardiaque normalisées qui sont relatives à des contractions auriculaires prématurées au moyen du procédé suivant,

dans lequel parmi les périodes de battement cardiaque normalisées $DR(N)_i$ issues d'une série chronologique R_i de périodes de battement cardiaque du coeur, une période de battement cardiaque normalisée $DR(N)_i$ qui satisfait les équations (5) et (6) suivantes est récupérée, et alors $DR(N)_i$ et la valeur $DR(N)_{i+1}$ qui la suit sont exclues de la période de battement cardiaque normalisée $DR(N)_i$ récupérée,

$$\frac{R_i + R_{i+1} - 2\bar{R}_{i-1}(M)}{2\bar{R}_{i-1}(M)} < 2T_A \quad \dots\dots (5)$$

$$\frac{(K+1)|R_{i-1} - R_{i+1}|}{K\bar{R}_{i-1}(K) + R_{i+1}} < T_N \quad \dots\dots (6)$$

dans lequel T_N et T_A sont des valeurs de seuil déterminées qui satisfont les relations $T_N > 0$ et $-T_N \leq T_A \leq 0$, l'indice i est une série chronologique, et i signifie le passé par rapport à $i+1$, M est un entier supérieur ou égal à 1, et K est un entier supérieur ou égal à 0, et $\bar{R}_i(X)$ dans les équations (5) et (6) est représenté par l'équation (7) suivante lorsque X est un entier supérieur

ou égal à 1, et par l'équation (8) suivante lorsque $X = 0$,

$$\bar{R}_i(X) = \frac{1}{X} \sum_{k=i-X+1}^i R_k \quad \dots\dots (7)$$

$$\bar{R}_i(0) = 0 \quad \dots\dots (8)$$

10. Système de détection de fibrillation auriculaire (1) selon l'une quelconque des revendications 1 à 9, dans lequel le système de détection de fibrillation auriculaire (8) est **caractérisé en ce que** le moyen de calcul de périodes de battement cardiaque normalisées est configuré pour calculer une période de battement cardiaque normalisée $DR(2)_n$, représentée par l'équation (9) suivante, à partir des périodes de battement cardiaque,

$$DR(2)_n = \frac{2(R_{n-1} - R_n)}{R_{n-1} + R_n} \quad \dots\dots (9)$$

11. Système de détection de fibrillation auriculaire (1) selon l'une quelconque des revendications 1 à 9, dans lequel le système de détection de fibrillation auriculaire (8) est **caractérisé en ce qu'il** comprend un capteur (19) pour mesure de battement cardiaque pourvu du moyen de mesure de périodes de battement cardiaque (4), et un analyseur pourvu du moyen de calcul de périodes de battement cardiaque normalisées (7), du moyen de cumul de périodes de battement cardiaque normalisées anormales (10) et du moyen de comparaison/détermination.

12. Système de détection de fibrillation auriculaire (1) selon la revendication 10, dans lequel le système de détection de fibrillation auriculaire (1) est **caractérisé en ce qu'il** comprend un capteur (19) pour mesure de battement cardiaque pourvu du moyen de mesure de périodes de battement cardiaque (4), et un analyseur pourvu du moyen de calcul de périodes de battement cardiaque normalisées (7), du moyen de cumul de périodes de battement cardiaque normalisées anormales (10) et du moyen de comparaison/détermination (12).

13. Système de détection de fibrillation auriculaire (1) selon la revendication 11, dans lequel le système de détection de fibrillation auriculaire (1) est **caractérisé en ce que** le capteur (19) est pourvu d'un moyen de stockage de périodes de battement cardiaque (14) destiné à stocker des périodes de battement cardiaque mesurées par le moyen de mesure de périodes de battement cardiaque (4), ou pourvu d'un moyen de transmission de périodes de battement cardiaque (5) destiné à transmettre à un analyseur les périodes de battement cardiaque mesurées, le système (1) étant configuré de telle sorte qu'une fibrillation auriculaire est détectée en entrant les périodes de battement cardiaque mesurées au moyen du capteur (19) dans l'analyseur via le moyen de stockage de périodes de battement cardiaque (14) ou le moyen de transmission de périodes de battement cardiaque (5).

14. Système de détection de fibrillation auriculaire (1) selon la revendication 12, dans lequel le système de détection de fibrillation auriculaire (1) est **caractérisé en ce que** le capteur (19) est pourvu d'un moyen de stockage de périodes de battement cardiaque (14) destiné à stocker des périodes de battement cardiaque mesurées par le moyen de mesure de périodes de battement cardiaque (4), ou pourvu d'un moyen de transmission de périodes de battement cardiaque (5) destiné à transmettre à un analyseur les périodes de battement cardiaque mesurées, le système (1) étant configuré de telle sorte qu'une fibrillation auriculaire est détectée en entrant les périodes de battement cardiaque mesurées au moyen du capteur (19) dans l'analyseur via le moyen de stockage de périodes de battement cardiaque (14) ou le moyen de transmission de périodes de battement cardiaque (5).

FIG. 1

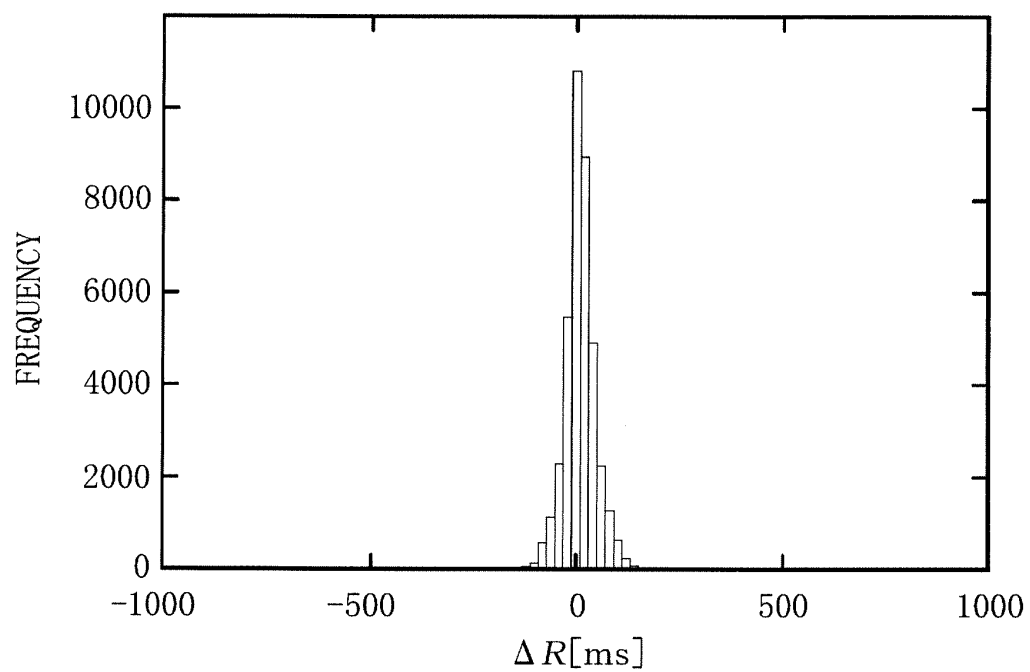


FIG. 2

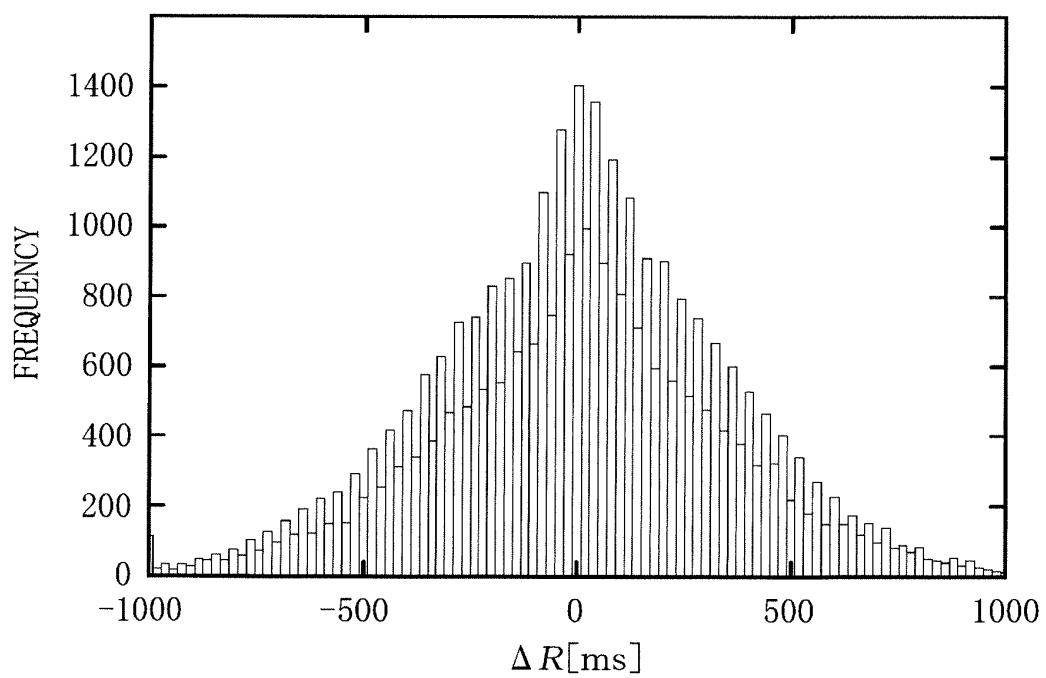


FIG. 3

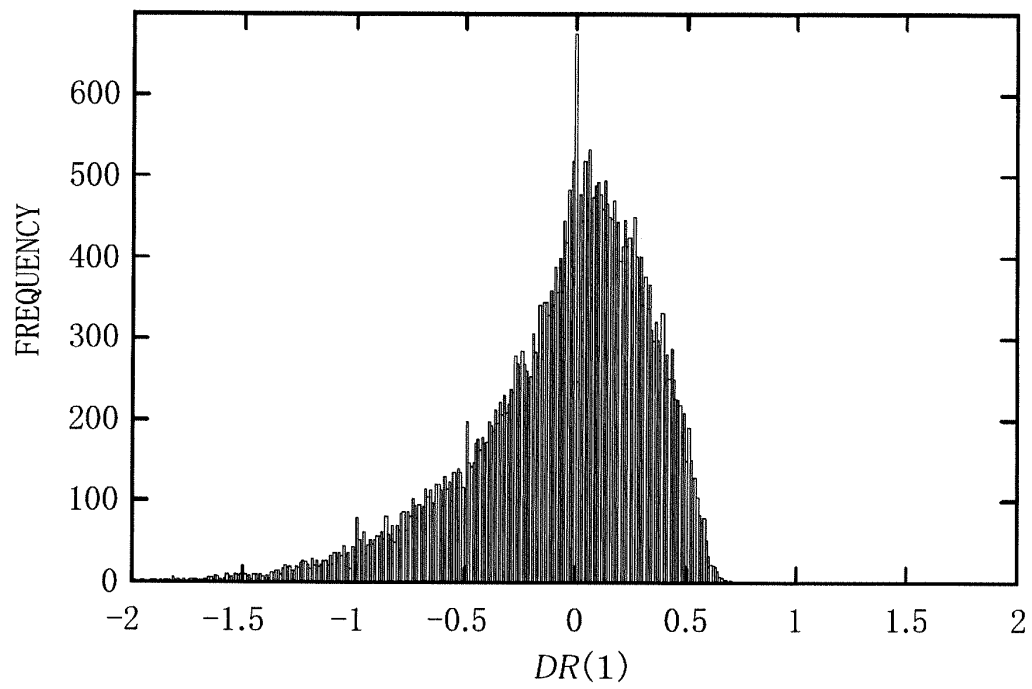


FIG. 4

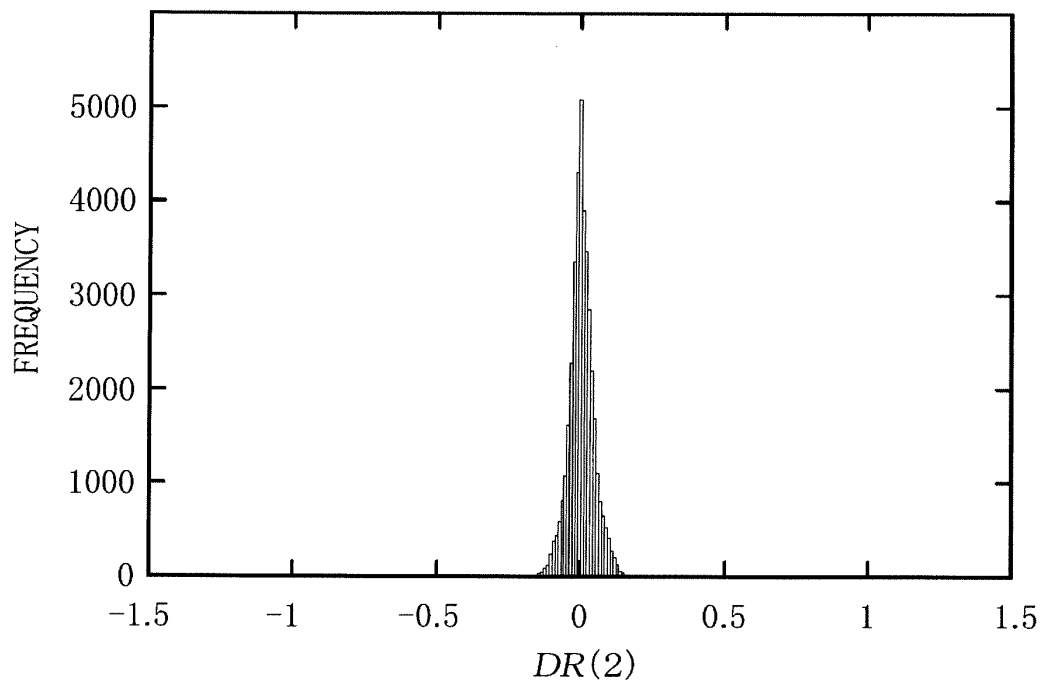


FIG. 5

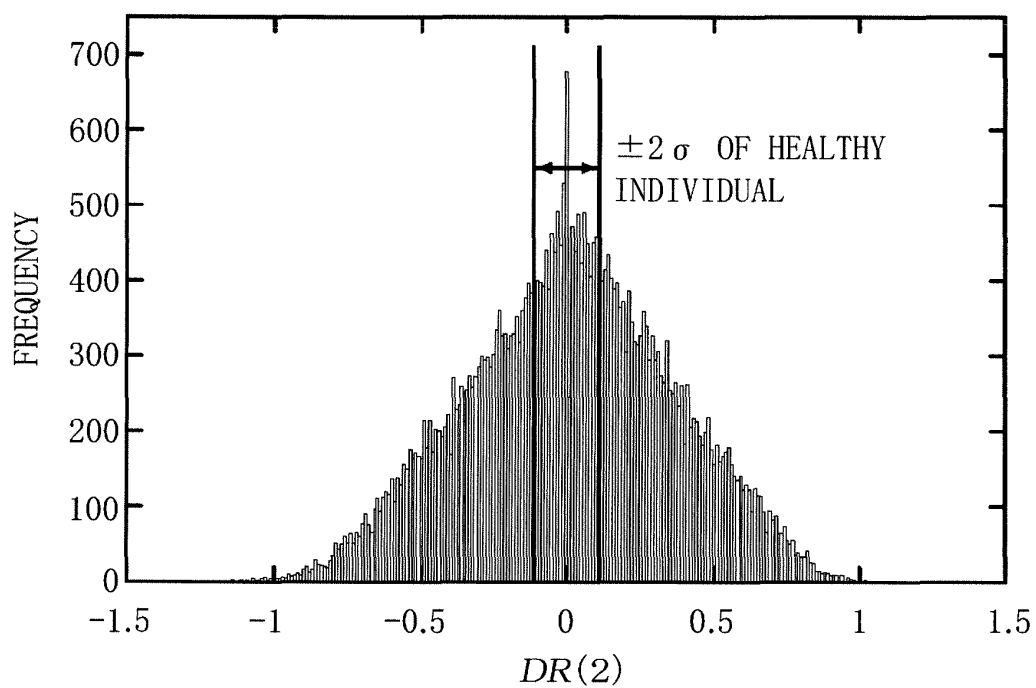


FIG. 6

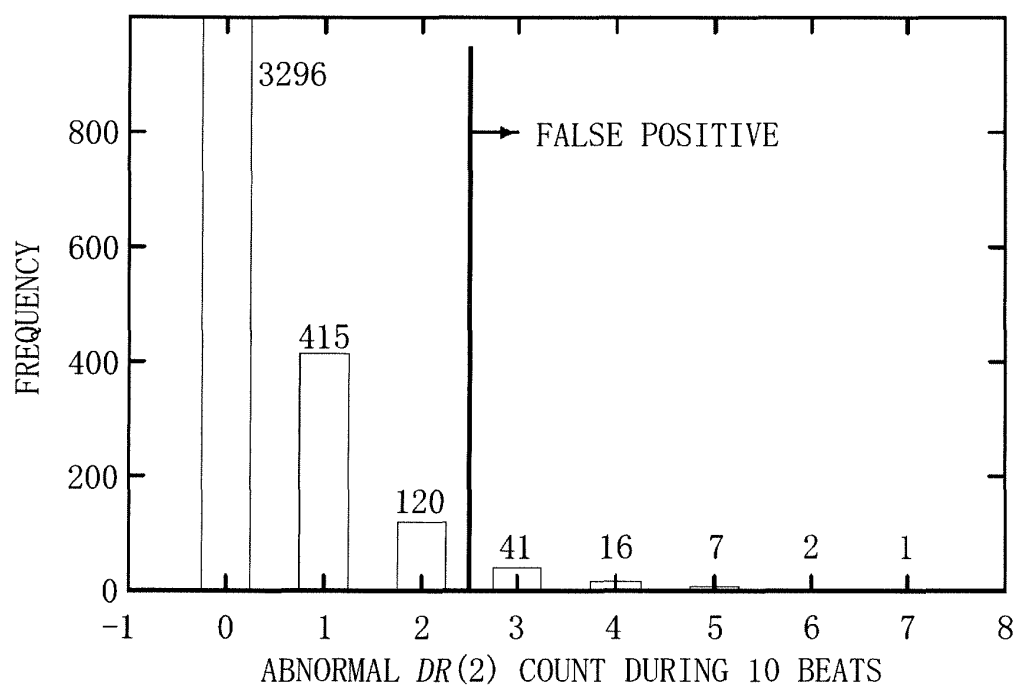


FIG. 7

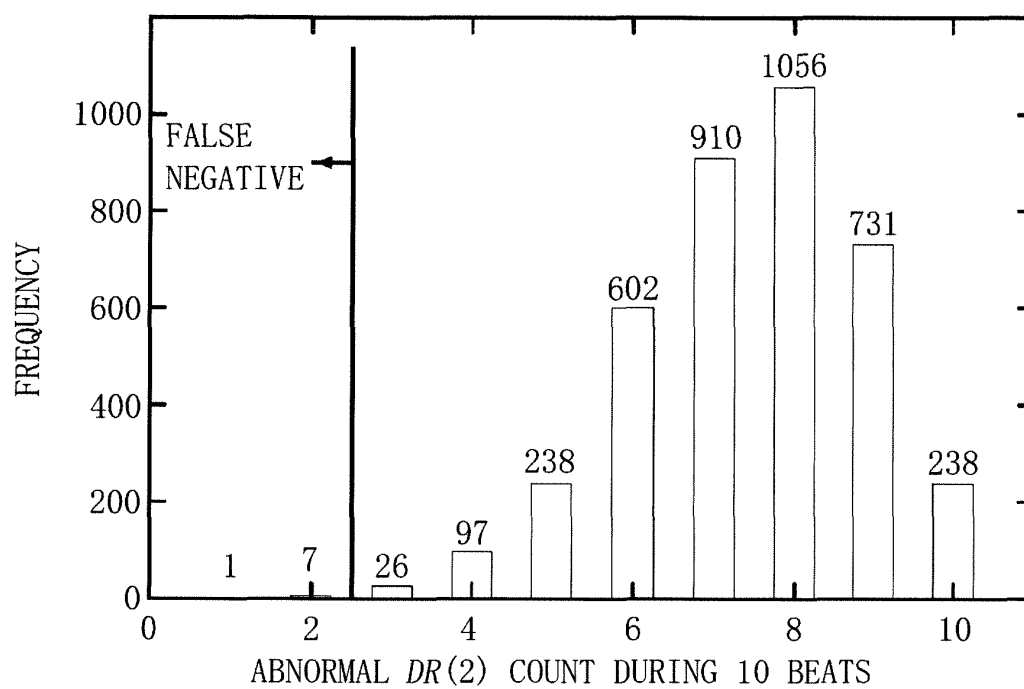


FIG. 8

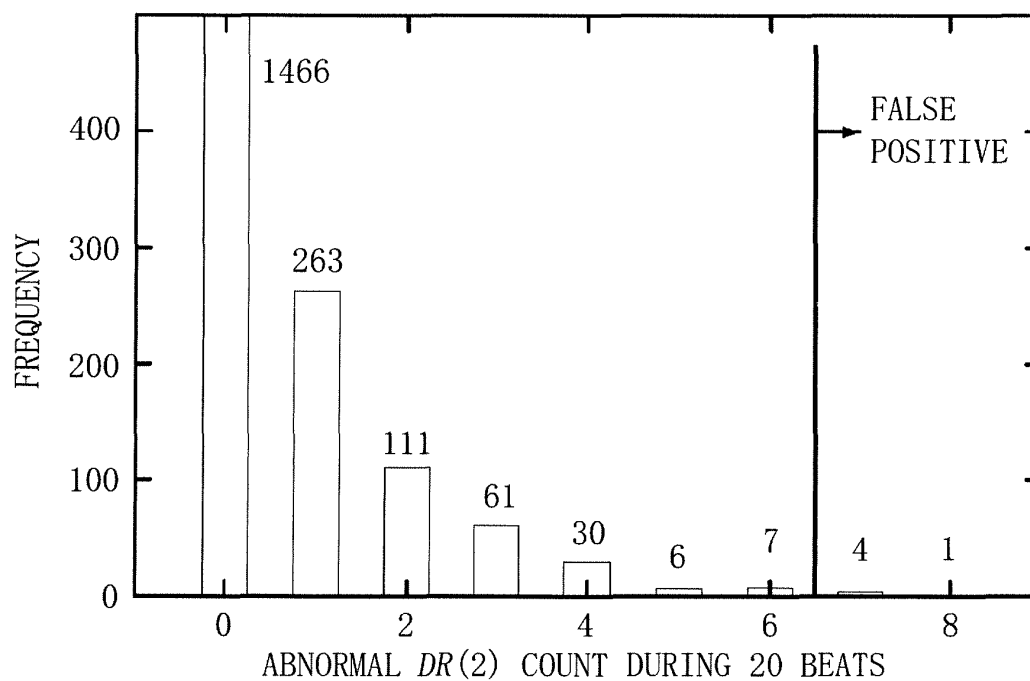


FIG. 9

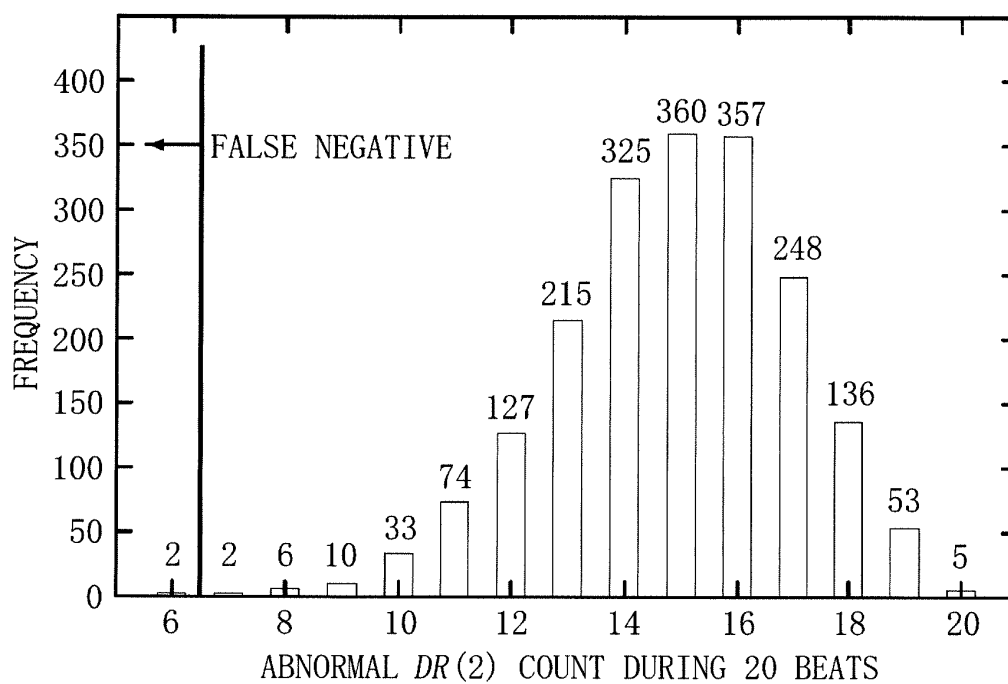


FIG. 10

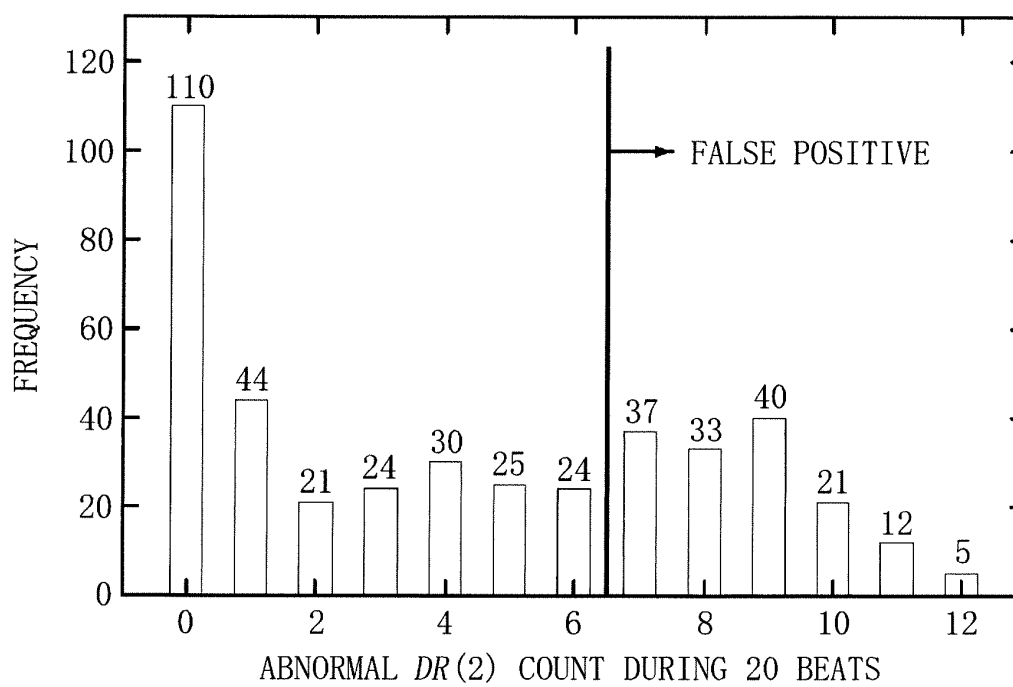


FIG. 11

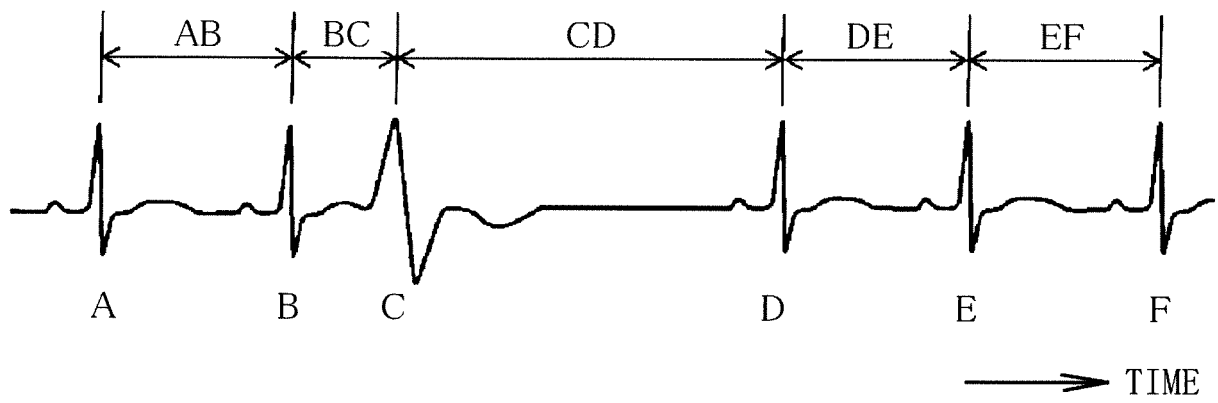


FIG. 12

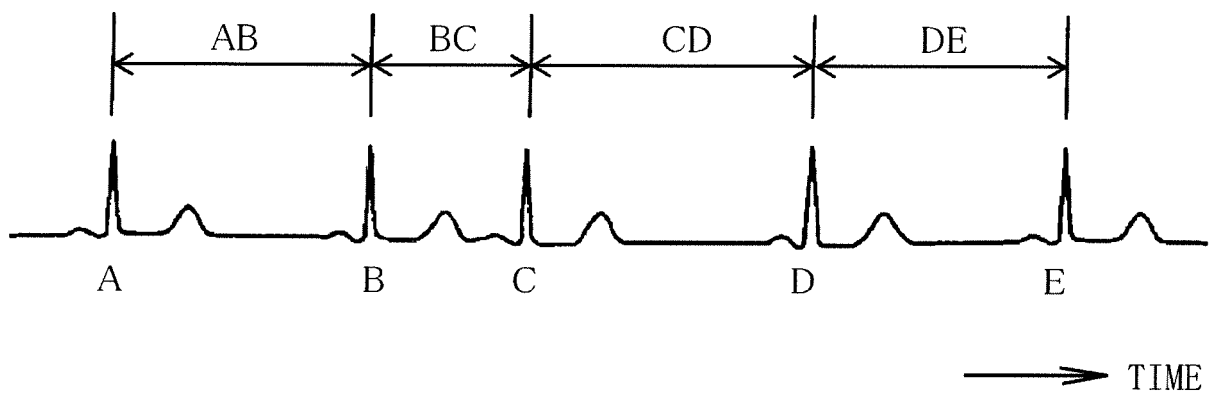


FIG. 13

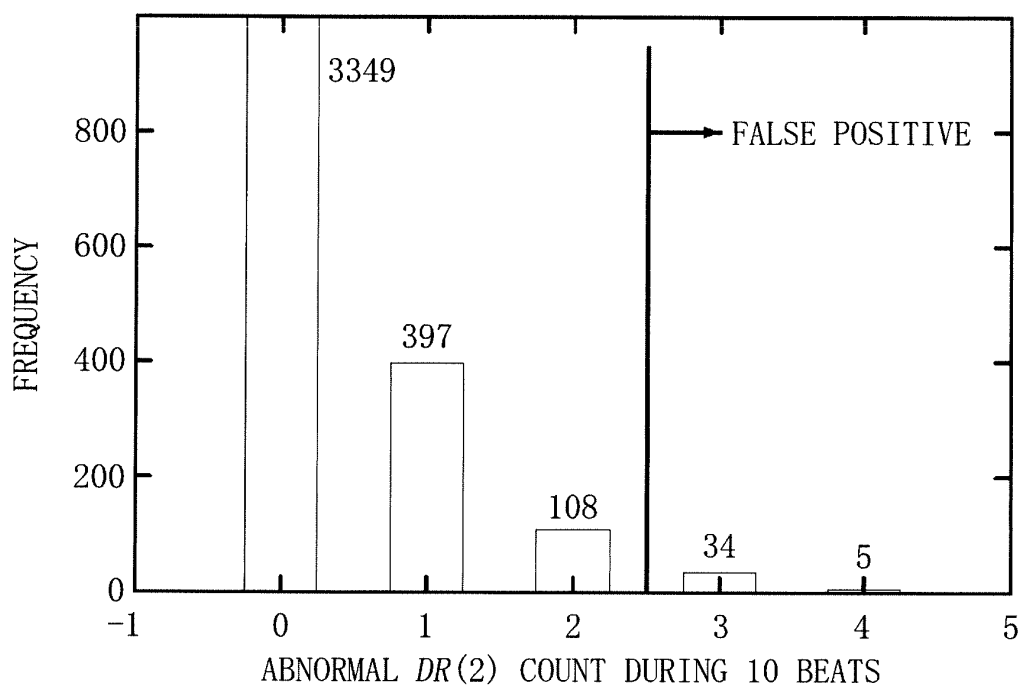


FIG. 14

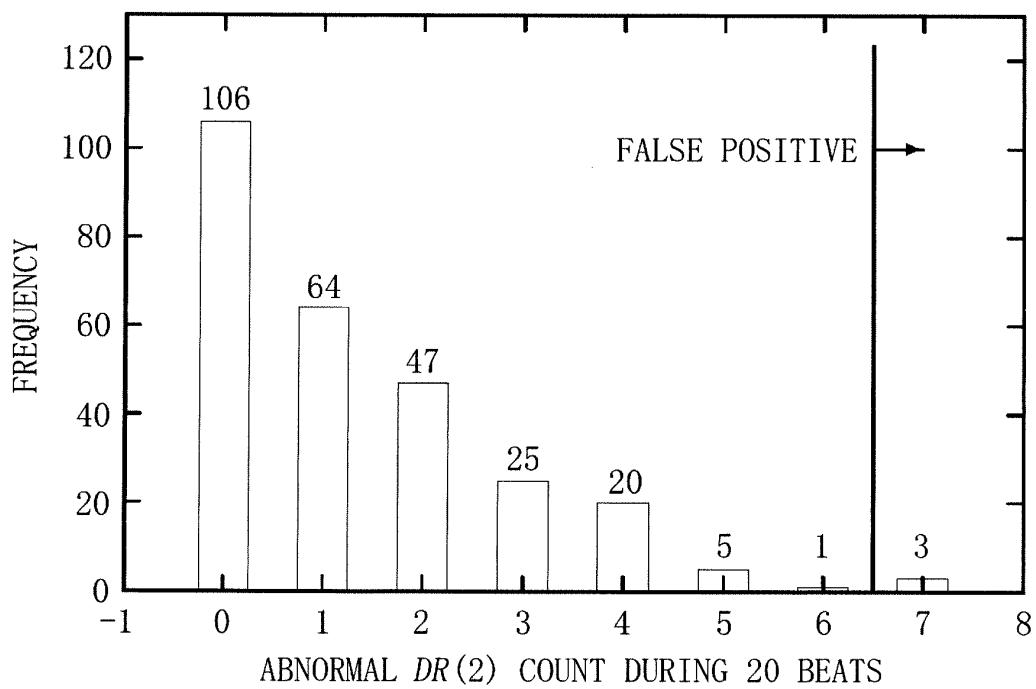


FIG. 15

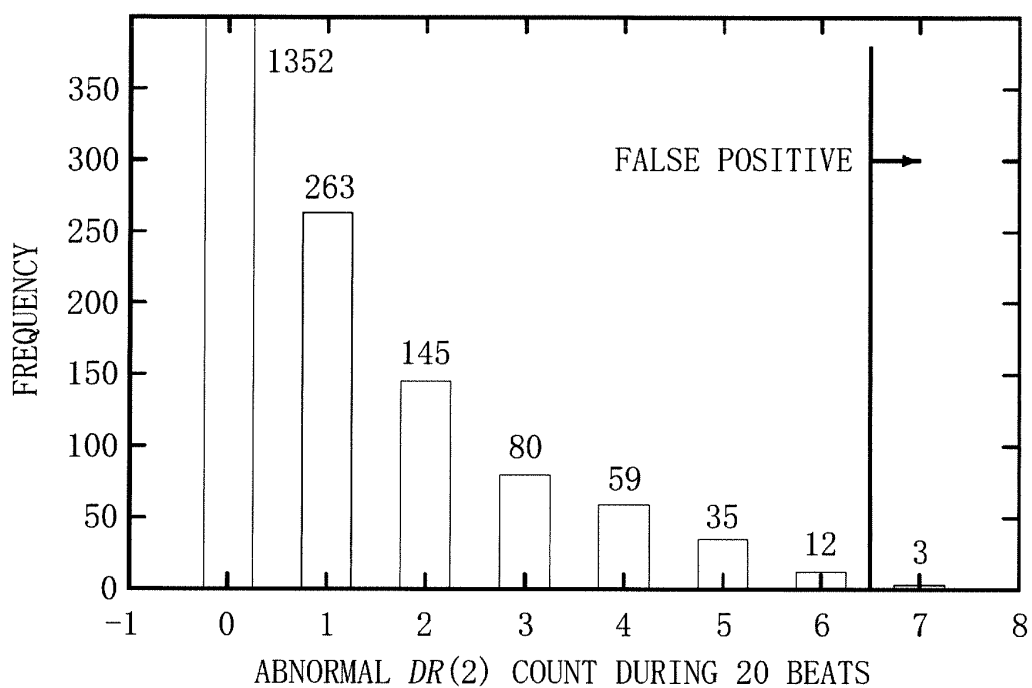


FIG. 16

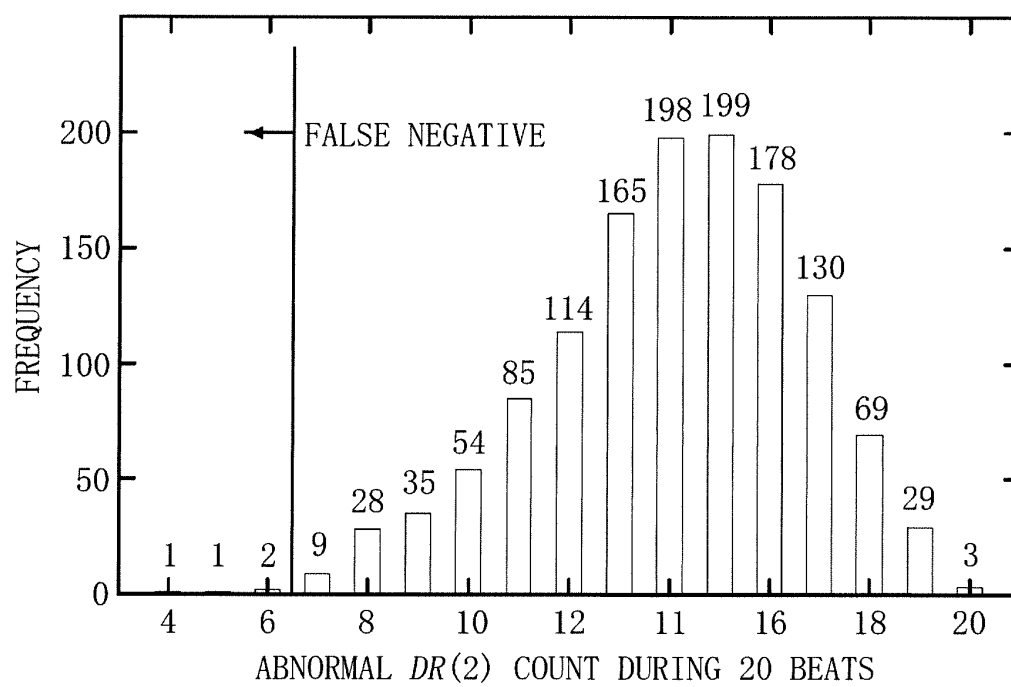


FIG. 17

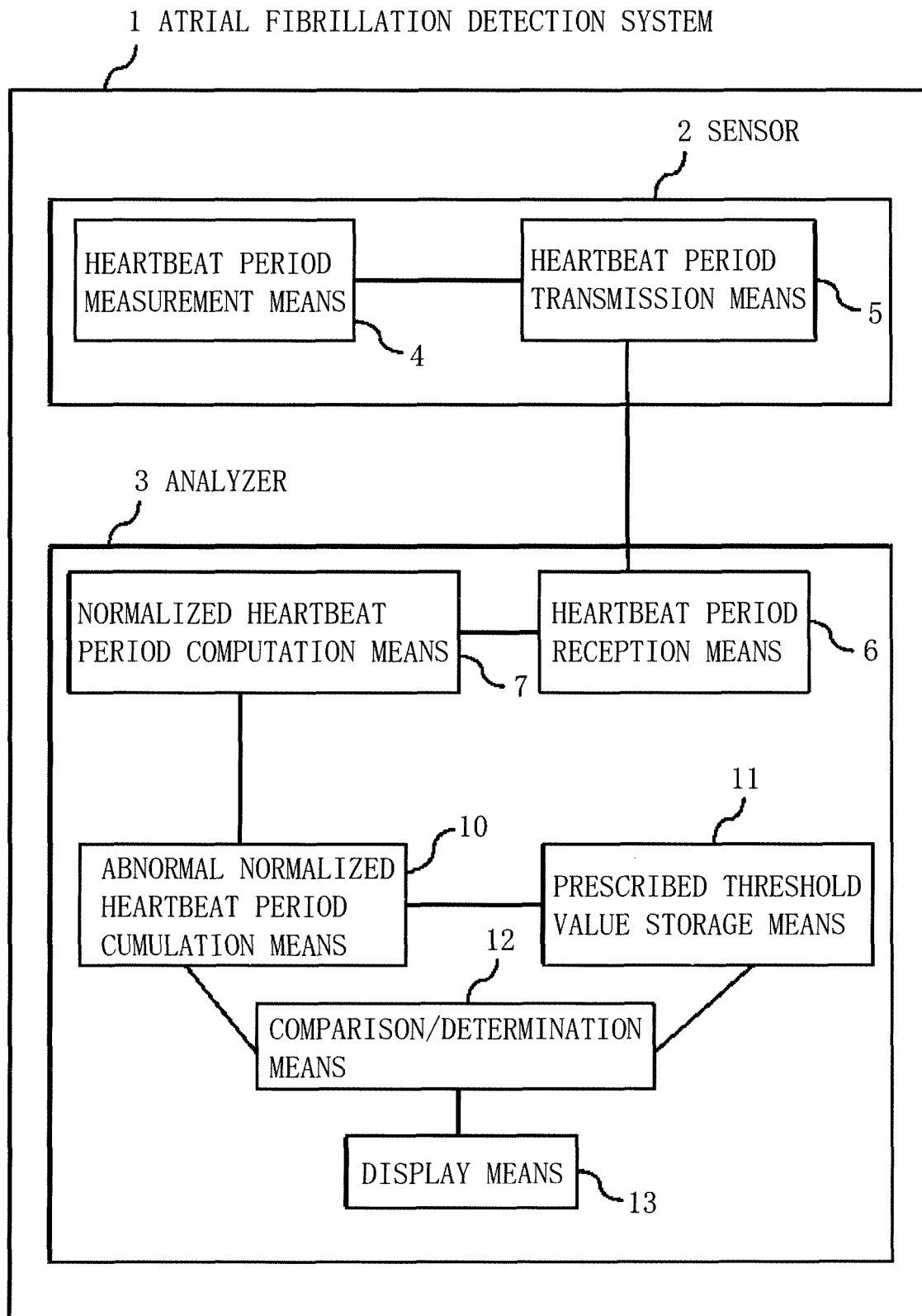


FIG. 18

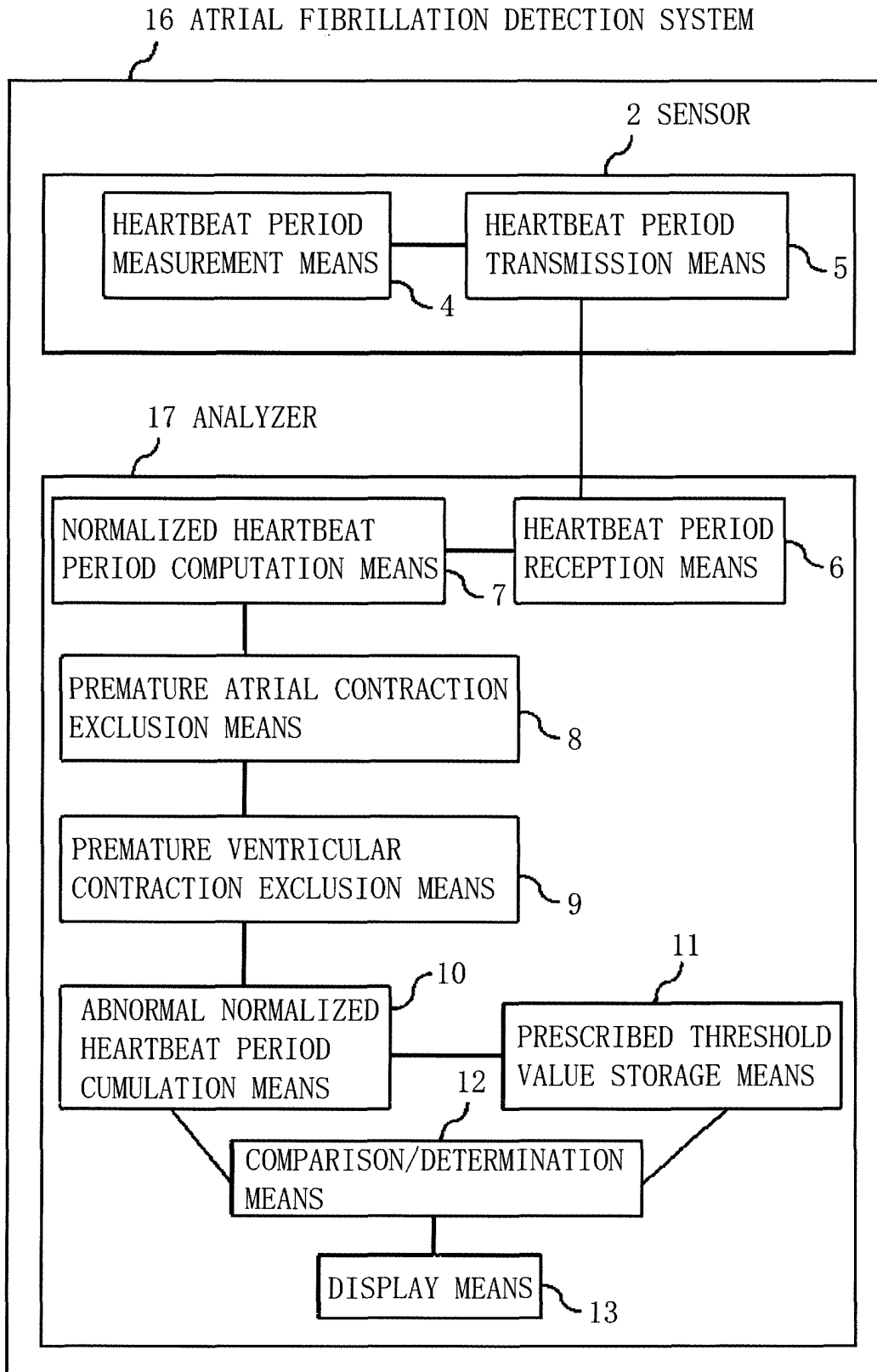
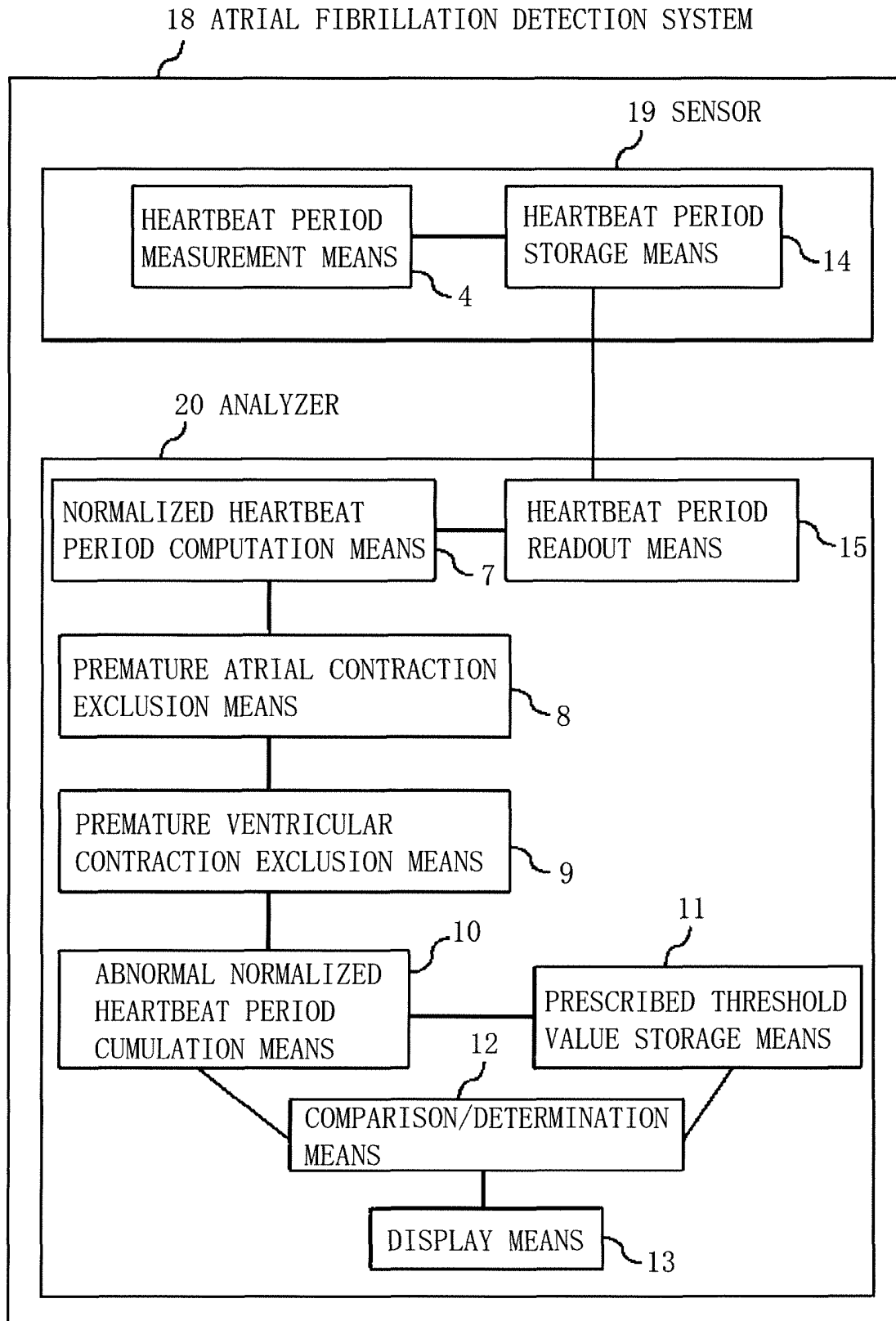


FIG. 19



REFERENCES CITED IN THE DESCRIPTION

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- JP 2009089883 A [0010]
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IPC分类号	A61B5/046 A61B5/024 A61B5/04 A61B5/00 A61N1/39		
CPC分类号	A61B5/04012 A61B5/046 A61B5/7271 A61B5/02405 A61B5/04014 A61N1/395 A61B5/0006		
优先权	2015021011 2015-02-05 JP		
其他公开文献	EP3053520A1		
外部链接	Espacenet		

摘要(译)

本发明提供一种心房颤动检测系统，其能够减轻对受试者的负担，通过该系统可以检测甚至阵发性心房颤动，并且可以在家中使用，有助于早期发现心房颤动。该心房颤动检测系统检测受试者中心房纤颤的存在，并提供测量心脏心跳周期的心跳周期测量装置;标准化心跳周期计算装置，计算由心跳周期测量装置测量的心脏心跳周期的标准化心跳周期DR (N);异常的归一化心跳周期累积意味着，从规定数量的连续归一化心跳周期DR (N) 中，将具有超过正常心跳周期值的绝对值的异常归一化心跳周期的计数相加;并且比较/确定意味着比较异常标准化心跳周期的累积计数和正常累积计数阈值，并且在异常标准化心跳周期的累积计数超过正常累积计数阈值的情况下，确定心房发生了原纤化。

$$DR(N)_n = \frac{N(R_{n-1} - R_n)}{\sum_{k=n-N+1}^n R_k} \dots$$