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(54) **MINIATURE FORWARD-LOOKING ULTRASOUND IMAGING MECHANISM ENABLED BY LOCAL SHAPE MEMORY ALLOY ACTUATOR**

NACH VORN WEISENDER MINIATUR-ULTRASCHALLBILDGEBUNGSMECHANISMUS, DER DURCH EIN LOKALES BETÄTIGUNGSELEMENT AUS EINER FORMGEDÄCHTNISLEGIERUNG AKTIVIERT WIRD

MÉCANISME MINIATURE D'IMAGERIE ULTRASONORE FRONTALE À ACTIONNEUR LOCAL EN ALLIAGE À MÉMOIRE DE FORME

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• **LEVY, Oren**
Emerald Hills, CA 94062 (US)

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(74) Representative: **de Haan, Poul Erik**
Philips International B.V.
Philips Intellectual Property & Standards
High Tech Campus 5
5656 AE Eindhoven (NL)

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(73) Proprietor: **Volcano Corporation**
San Diego, CA 92130 (US)

(72) Inventors:

• **PARK, Byong-Ho**
Cincinnati
OH 45230 (US)

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Description

BACKGROUND

Field

[0001] Embodiments disclosed herein concern a miniature actuator which is useful in intravascular imaging devices including intravascular ultrasound (IVUS), and optical coherence tomography (OCT). The miniature actuator mechanism and ultrasound or OCT imaging device is preferably embedded in an elongated body such as an intravascular guide wire or catheter to provide imaging guidance in various interventional applications.

Description of the Related Art

[0002] Coronary artery disease is very serious and often requires an emergency operation to save lives. The main cause of coronary artery disease is the accumulation of plaque inside a person's vasculature, which eventually occludes blood vessels. Several solutions are available, for example, balloon angioplasty, rotational atherectomy, and intravascular stents, to open up the clogged section, which is called stenosis. Traditionally, during the operation, surgeons rely on X-ray fluoroscopic images that are basically planary images showing the external shape of the silhouette of the lumen of blood vessels. Unfortunately, with X-ray fluoroscopic images, there is a great deal of uncertainty about the exact extent and orientation of the atherosclerotic lesions responsible for the occlusion, making it difficult to find the exact location of the stenosis. In addition, though it is known that restenosis can occur at the same place, it is difficult to check the condition inside the vessels after surgery. Intravascular imaging would be valuable during interventional procedures to facilitate navigation and for intraoperative feedback. For example, the precise placement and appropriate expansion of stents would benefit from simultaneous intravascular imaging. Existing intravascular imaging devices are too large and are not flexible enough to be placed simultaneously with other devices.

[0003] In order to resolve these issues, an ultrasonic transducer device has been utilized for endovascular intervention to visualize the inside of the blood vessels. To date, the current technology is mostly based on one or more stationary ultrasound transducers or rotating a single transducer in parallel to the blood vessels by means of a rotating shaft which extends through the length of the catheter to a motor or other rotary device located outside the patient. These devices have limitations in incorporating other interventional devices into a combination device for therapeutic aspects. They require a large space inside catheter such that there is not enough room to accommodate other interventional devices. Also, due to the nature of the rotating shaft, the distal end of the catheter is very stiff and it is hard to navigate through tortuous arteries. The high speed rotating shaft also contributes to distorted non-uniform images when imaging a tortuous path in the vasculature. OCT has also been utilized to visualize the intravascular space based on differential reflectance, but most existing OCT devices rely on a rotating fiber optic which extends along the length of the device. This approach also has problems, for example, the manipulation, spinning and scanning motion required with respect to a delicate glass or polycarbonate optical fiber; the actuator mechanism located outside the patient and tip located inside the patient are significantly distant from one another, leading to inefficiencies and control issues arising from the torque created by a long, spinning member; and remote mechanical manipulation and a long spinning element distort the image due to non-uniform rotational distortion.

[0004] Additionally, current devices are mainly side-looking devices that are not able to provide valuable information to be used as guidance during invasive procedures. Forward-looking ultrasound imaging is essential in guiding an interventional device for treatment in a timely manner. For example, when implanting a heart pacemaker, electrical leads need to be implanted in precise locations. Currently there is no accurate forward-looking imaging device to direct the leads to the right locations. Thus, physicians are required to blindly rely on guide catheters and spend more time than needed when performing procedures. Also, patients are being over exposed to unnecessary radiation and toxic contrast agents involved with fluoroscopy. Given the numerous difficulties with current intravascular imaging devices, there is a need for an improved forward-looking intravascular imaging device.

[0005] A forward-looking intravascular ultrasound device is known from document US 5 379 772 A.

SUMMARY

[0006] One embodiment of the invention is a forward-looking intravascular ultrasound device that includes an ultrasound transducer that rotates around an axis of rotation and a local actuator configured to cause the ultrasound transducer to rotate. The linear actuator includes a movable element that moves back and forth from a first position to a second position. The movable element is connected to at least one SMA actuator that is expands or contracts when activated in order to move the movable element from the first position to the second position or from the second position to the first position. The movable element engages the ultrasound transducer and causes it to rotate around the axis of rotation

to create a forward-looking sweeping motion. The ultrasound transducer may continue to rotate even after it disengages from the movable element due to the moment of inertia of the transducer or some other amplifying force, for example, a biasing force.

[0007] One embodiment of the invention is a forward-looking intravascular ultrasound device comprising an elongated body having a longitudinal end, an interior surface, an exterior surface, a proximal end, and a distal end; an ultrasound transducer element disposed at least partially in the distal end of the elongated body and configured to rotate between at least a primary position and a secondary position about an axis of rotation that is generally normal to the longitudinal axis; and a local actuator comprising a first element, wherein the first element is secured to and does not move relative to the body; a movable element, wherein the movable element is configured to move longitudinally substantially parallel to the longitudinal axis between at least a first position and a second position, wherein the movable element is configured to engage the ultrasound transducer element at least when the movable element moves from the first position to the second position; a first SMA actuator coupled to the first element and the movable element, wherein the first SMA actuator is configured to switch between an activated and deactivated state, wherein the movable element moves from the first position to the second position upon activation of the first SMA actuator; and wherein the ultrasound transducer element rotates about the axis of rotation at least when the movable element and the ultrasound transducer element are engaged and the movable element moves from the first position to the second position. In another embodiment, the device comprises a biasing element coupled to the movable element and the first element, wherein the biasing element is configured to move the movable element from the second position to the first position. In yet another embodiment, the biasing element comprises a spring.

[0008] In another embodiment, the device described herein comprises a second element, wherein the second element is secured to and does not move relative to the body; and a biasing element coupled to the second element and the movable element, wherein the biasing element is configured to move the movable element from the second position to the first position. In some embodiments, the first and second elements are disposed along an axis that is substantially parallel to the longitudinal axis. In other embodiments, the first and second elements are disposed along an axis that is substantially normal to the longitudinal axis. In some embodiments, the biasing element comprises a spring. In other embodiments, the biasing element comprises a second SMA actuator, wherein the second SMA actuator has an activated and a deactivated state and when the second SMA actuator is activated it opposes motion of the movable element from the first position to the second position. In some embodiments, the cross-sectional shape of the distal end of the body is generally curvilinear and has a diameter of not more than about 5.08 mm (0.200 inches).

[0009] Some embodiments of the device comprise an electrical wire connected to the ultrasound transducer element. In some embodiments, the device comprises a member coupled with the interior surface of the elongated body at or near the distal end, wherein the ultrasound transducer element is configured to rotate about the member between at least the primary position and the secondary position. In some embodiments, the electrical wire is coiled at least partially around the member. In some embodiments, the cam and ultrasound transducer element are not continuously engaged while the movable element moves from the second position to the first position.

[0010] In some embodiments, the angle of rotation the ultrasound transducer element rotates about the axis of rotation between the primary position and the secondary position is between about 5° and about 185°. In some embodiments, the angle of rotation the ultrasound transducer element rotates about the axis of rotation when the movable element moves from the first position to the second position is less than the angle of rotation the ultrasound transducer element rotates about the axis of rotation between the primary position and the secondary position. In some embodiments, the linear actuator is not fixed to the ultrasound transducer element. In some embodiments, the ultrasound transducer and cam are not engaged after the movable element reaches the second position and the ultrasound transducer continues to rotate about the axis of rotation towards the secondary position. In some embodiments, the ultrasound transducer element comprises a biasing element configured to bias the ultrasound transducer towards the secondary position. In some embodiments, the biasing element comprises a spring. In some embodiments, the biasing element comprises an electrical wire. In some embodiments, the ultrasound transducer element comprises a high density material and a transducer crystal. In some embodiments, the volume of the ultrasound transducer element is at least about 0.1 cubic mm. In some embodiments, the mass of the ultrasound transducer element is at least about 1 mg. In some embodiments, the ultrasound transducer element is configured to transmit ultrasound energy at an angle of between about 15° and 165° relative to an axis that is generally normal to the longitudinal axis and the axis of rotation. In some embodiments, the elongated body comprises a guide wire. In some embodiments, the first element comprises an aperture, and the movable element is disposed at least partly within the aperture. In some embodiments, the movable element comprises a shaft and in some embodiments, the movable element comprises a shaft connected to a cam.

[0011] Another embodiment is a method of visualizing the interior of a patient's vascular, the method comprising inserting the distal end of a device disclosed herein into the vasculature of the patient; generating an ultrasound signal from the ultrasound transducer element; activating the first SMA actuator such that the movable element moves from the first position to the second position and the cam engages the ultrasound transducer element; deactivating the first SMA actuator such that the biasing element moves the movable element from the second position to the first

position; receiving an ultrasound signal reflected from the interior of the vasculature on the ultrasound transducer element; and producing an image from the reflected signal.

[0012] Also disclosed herein is a forward-looking intravascular ultrasound device comprising an elongated body having a longitudinal axis, an exterior surface, a proximal end, and a distal end; an ultrasound transducer means disposed in the distal end of the elongated body and configured to rotate about an axis of rotation that is generally normal to the longitudinal axis; and a local actuator means configured to engage the ultrasound transducer means and cause the ultrasound transducer means to rotate about the axis of rotation at least when the local actuator means and ultrasound transducer means are engaged.

BRIEF DESCRIPTION OF THE DRAWINGS

[0013]

Figure 1A is a partial cut-away perspective view showing an embodiment of a forward-looking ultrasound imaging device.

Figure 1B is a partial cut-away side view of the forward-looking ultrasound imaging device depicted in Figure 1A.

Figure 2A is a partial cut-away perspective view showing an embodiment of a local actuator including a movable element.

Figure 2B is a partial cut-away perspective view showing the local actuator depicted in Figure 2A with the movable element in a different position than shown in Figure 2A.

Figure 2C is a partial cut-away side view showing an embodiment of a local actuator.

Figure 2D is a partial cut-away side view showing an embodiment of a local actuator.

Figure 2E is a partial cut-away side view showing an embodiment of a local actuator.

Figure 3A is a diagram showing how the rotational motion of a SMA actuator is controlled.

Figure 3B is a diagram showing how the longitudinal motion of a SMA actuator is controlled.

Figure 4A is a perspective view of an embodiment of an ultrasound transducer element configured to rotate about a coupling member.

Figure 4B is a side view of an embodiment of an ultrasound transducer element.

Figure 4C is a side view of an embodiment of an ultrasound transducer element.

Figure 5 is a partial cut-away side view of an embodiment of a forward-looking ultrasound imaging device.

Figure 6A is a partial cut-away side view of an embodiment of a forward-looking ultrasound imaging device.

Figure 6B is a partial cut-away side view of the forward-looking ultrasound imaging device shown in Figure 6A showing the ultrasound transducer element in a different position.

Figure 6C is a partial cut-away side view of the forward-looking ultrasound imaging device shown in Figure 6B showing the ultrasound transducer element in a different position.

Figure 7A is a partial cut-away side view of an embodiment of a forward-looking ultrasound imaging device.

Figure 7B is a partial cut-away side view of the forward-looking ultrasound imaging device shown in Figure 7A showing the ultrasound transducer element in a different position.

Figure 7C is a partial cut-away side view of the forward-looking ultrasound imaging device shown in Figure 7B showing the ultrasound transducer element in a different position.

Figure 7D is a partial cut-away side view of the forward-looking ultrasound imaging device shown in Figure 7C showing the ultrasound transducer element in a different position.

Figure 8A is a partial cut-away side view of an embodiment of a forward-looking ultrasound imaging device.

Figure 8B is a partial cut-away side view of the forward-looking ultrasound imaging device shown in Figure 8A showing the ultrasound transducer element in a different position.

Figure 9A is a diagram showing waveforms of voltage versus time that is used to produce different scanning motions for a transducer element in a forward-looking imaging device.

Figure 9B is a diagram showing the angle of rotation versus time for a transducer element in a forward-looking imaging device during an active path and returning path.

Figure 10A is a perspective view of an embodiment of a forward-looking ultrasound imaging device.

Figure 10B is a partial cut-away perspective view of an embodiment of a forward-looking ultrasound imaging device.

Figure 10C is a partial cut-away side view of an embodiment of a forward-looking ultrasound imaging device.

DETAILED DESCRIPTION

[0014] Embodiments disclosed herein relate to imaging devices for intravascular imaging, although the present invention is not limited to this preferred application. Imaging of the intravascular space, particularly the interior walls of the vasculature can be accomplished by a number of different means. Two of the most common are the use of ultrasound

energy, commonly known as intravascular ultrasound (IVUS) and optical coherence tomography (OCT). Both of these methods are optimized when the instruments (IVUS or OCT) used for imaging a particular portion of the vasculature are repeatedly swept over the area being image, for example, with a back and forth sweeping motion or rotational sweeping motion.

[0015] To address the limitations in current devices, a new intravascular imaging device is described based on a Shape Memory Alloy (SMA) actuator device embedded inside an elongated body such as a guide wire or catheter. Embodiments of the present invention utilizes a novel SMA device to provide forward-looking imaging by providing movement for an ultrasound transducer or OCT element. Since this novel SMA actuator device can be easily fabricated in micro-scale using laser machining or other fabrication techniques, it provides an advantage over existing imaging devices because it offers the ability to miniaturize the overall size of the device, while the use of multiple transducer crystals maximizes field of view. The small dimensions of the actuator device of the invention allow for the cross-sectional area of the elongated body in which it is housed to be very small. The outside width of the elongated body, such as a guide wire or catheter containing an imaging device described herein can be as small as from about 0.0050" to about 0.200". The outside width for elongated bodies can be larger when the imaging device is combined with other interventional devices, although the outside width of these devices can be as small as 0.060" or smaller. Current catheters containing IVUS range from 0.70mm to 3mm in outside diameter.

[0016] Additionally, embodiments of the present invention address limitations stemming from fatigue failure due to the range of displacement in SMA actuator devices. Ultrasound devices must be able to operate for a certain period of time when used in invasive procedures. However, the life of the SMA actuator may be limited by fatigue failure after a certain amount of cycles of scanning. Fatigue failure can be delayed if the range of displacement the SMA actuator undergoes is limited. On the other hand, a large scanning motion is required to produce quality images during an invasive procedure. Embodiments disclosed herein balance these two concerns and incorporate an SMA actuator that undergoes a small displacement and applies an impulse force on the transducer. The transducer continues to rotate after the SMA actuator applies the impulse force due to the moment of inertia of the transducer and/or another biasing force, for example, a spring. Thus, embodiments disclosed herein can produce a large scanning motion while limiting the displacement of the SMA actuator and preventing or delaying fatigue failure of the SMA actuator

[0017] Existing single-element ultrasound (IVUS) devices are based on a rotating shaft with a driving motor located externally. An imaging tip with a transducer or mirror is mounted directly on the rotating shaft. As a result, when the rotating shaft has a slight change in its motion, it induces a non-uniform rotational distortion (NURD) in the actual image. NURD may happen when there is a kink along the length of the rotating shaft. Since shafts in current IVUS devices are relatively big, they tend to kink when going through a tortuous path, for example, a vasculature, resulting in a NURD problem in imaging. NURD happens in some instances because there is no way of knowing where the imaging tip is pointing if the device is not forward-looking. NURD can be reduced or eliminated if there is a feedback signal available from the distal end as provided in some embodiments disclosed herein.

[0018] Embodiments disclosed in this application do not require a rotating shaft or fiber optic along the length of the catheter, allowing for a more flexible catheter or guide wire, and providing room for other interventional devices. In addition, the lack of a rotating shaft eliminates the problems mentioned above with current OCT technology, for example, NURD. Another advantage of some of the embodiments disclosed herein is the elimination of non-uniform distortion of the acquired image that occurs in current IVUS devices. In one embodiment, the imaging mechanism (e.g., ultrasound transducer element) is located at the distal end of the device and does not continuously rotate but oscillates back and forth in a rotational sweeping motion. Additionally, an optional miniature spring can be embedded in the imaging mechanism and work as a position sensor or strain gauge to provide a feedback signal to the imaging system.

[0019] As used herein, "elongated body" includes any thin, long, flexible structure which can be inserted into the vasculature of a patient. Elongated bodies include, for example, intravascular catheters and guide wires. The local actuator is disposed in the distal end of the elongated body. As used herein, "distal end" of the elongated body includes the portion of the elongated body that is first inserted into the patient and is typically the most distant from the point of insertion after the elongated body enters the patient. As elongated bodies can be solid, some will include a housing portion at the distal end for receiving the local actuator. Such housing portions can be tubular structures attached to the side of the distal end or attached to the distal end of the elongated body. Other elongated bodies are tubular and have one or more lumens in which the actuator mechanism can be housed at the distal end.

[0020] "Connected" and variations thereof as used herein include direct connections, such as being glued or otherwise fastened directly to, on, within, etc. another element, as well as indirect connections where one or more elements are disposed between the connected elements.

[0021] "Secured" and variations thereof as used includes methods by which an element is directly secured to another element, such as being glued or otherwise fastened directly to, on, within, etc. another element, as well as indirect means of securing two elements together where one or more elements are disposed between the secured elements.

[0022] Movements which are "counter" are movements in the opposite direction. For example, if the ultrasound transducer element is rotated clockwise, rotation in a counterclockwise direction is a movement which is counter to the

clockwise rotation. Similarly, if the movable element is moved substantially parallel to the longitudinal axis of the elongate member in a distal direction, movement substantially parallel to the longitudinal axis in a proximal direction is a counter movement.

[0023] As used herein, "light" or "light energy" encompasses electromagnetic radiation in the wavelength range including infrared, visible, ultraviolet, and X rays. The preferred range of wavelengths for OCT is from about 400nm to about 1400nm. For intravascular applications, the preferred wavelength is about 1200 to about 1400nm. Optical fibers include fibers of any material which can be used to transmit light energy from one end of the fiber to the other.

[0024] Embodiments of the invention will now be described with reference to the accompanying Figures, wherein like numerals refer to like elements throughout. The terminology used in the description presented herein is not intended to be interpreted in any limited or restrictive manner, simply because it is being utilized in conjunction with a detailed description of certain specific embodiments of the invention. Furthermore, embodiments of the invention can include several novel features, no single one of which is solely responsible for its desirable attributes or which is essential to practicing the inventions herein described.

[0025] Figures 1A and 1B illustrate an embodiment of a novel forward-looking intravascular ultrasound device **100** capable of sweeping or scanning forward of the distal end of the device **100** to produce IVUS or OCT images. As shown in Figure 1A, the device **100** may include an elongated body **101** having a distal end, a proximal end, and a longitudinal axis. The elongated body **101** is any size. In one embodiment, the elongated body **101** is small enough to fit inside a standard guide catheter with an inner diameter that is, is about, is not less than, is not less than about, is not more than, or is not more than about 12Fr, 11Fr, 10Fr, 9Fr, 8Fr, 7Fr, 6Fr, 5Fr, 4Fr, 3Fr, 2Fr, 1Fr, or falls within a range defined by, and including, any two of these values. Thus, the outside diameter of the elongated body **101** is preferably less than the inner diameter of the standard guide catheter in some embodiments.

[0026] The elongated body **101** has at least a portion **107** which is at least partially sonolucent (e.g., permits the passage of at least some ultrasound waves without absorbing or reflecting them back to their source). The portion **107** can be a window made of an ultrasound transparent material, a material which is partially or substantially transparent to ultrasound energy, or the portion **107** can be a window, opening, or aperture. In some embodiments, the entire elongated body **101** or the majority of the distal end of the elongated body **101** is formed of a substantially sonolucent material.

[0027] In some embodiments, portions of the elongate member **101** are solid and other portions, for example, the distal end, include housing portions capable of receiving other objects. Such housing portions can be tubular structures attached to the side of the distal end or attached to the distal end of the elongated body **101**. Other elongated bodies **101** are tubular and have one or more lumens capable of housing other objects in the distal end. The elongated body **101** shown in Figures 1A and 1B houses an ultrasound transducer element **105**, a local actuator **103**, a coupling member **111**, and an electrical wire **109**. In some embodiments, the electrical wire **109** is connected to the ultrasound transducer element **105** and wrapped at least partially around the coupling member **111**. In some embodiments, the transducer element **105** comprises, or is secured directly or indirectly to the coupling member **111**.

[0028] The local actuator **103** is configured to engage (e.g., contact, push, or pull) the ultrasound transducer element **105** and cause the ultrasound transducer element **105** to rotate in a first direction and/or a second direction counter to the first direction about an axis of rotation. In some embodiments, the axis of rotation is generally normal to the longitudinal axis. In some embodiments, the ultrasound transducer element **105** is directly connected or coupled with the elongated body **101** and configured to rotate relative to the elongated body **101** about an axis of rotation. In some embodiments, the axis of rotation is substantially parallel to the coupling member **111**. In other embodiments, the ultrasound transducer element **105** is coupled with a member **111** that extends from an interior surface of the elongated member **101** such that the ultrasound transducer element **105** rotates about the member **111**.

[0029] Figures 2A and 2B show an embodiment of a local actuator **103** that includes a first element **205** and a second element **213** which are secured relative to the interior of the elongated body **101** to anchor or hold the device **103** in place relative to the elongated body **101** such that the first element **205** and second element **213** do move relative to the elongated body **101**. In some embodiments, the first and second elements **205**, **213** are disposed anywhere within the elongated body **101**, for example, at or near the distal end.

[0030] In some embodiments, the local actuator **103** includes a movable element **209** that is configured to move relative to the first element **205**, the second element **213**, and the elongated body **101**. In some embodiments, the movable element **209**, the first element **205**, and the second element **213** are disposed along an axis within the elongated body **101**, for example, an axis that is substantially parallel to the longitudinal axis. In one embodiment, the movable element **209**, the first element **205**, and the second element **213** are disposed along an axis that is substantially normal to the longitudinal axis or an axis that is substantially not parallel to the longitudinal axis. In some embodiments, the movable element **209** is disposed between the first element **205** and the second element **213** and configured to move between the first element **205** and the second element **213**. In one embodiment, the movable element **209** moves in a first direction along an axis that is substantially parallel to the longitudinal axis and in a second direction that is counter to the first direction. In another embodiment, the movable element **209** is configured to move in more than one range of

motion, for example, along an axis that is substantially parallel to the longitudinal axis as well as rotationally about the longitudinal axis.

[0031] In one embodiment, the first element **205** is connected or coupled with the movable element **209** by a first shape memory alloy (SMA) actuator **207** which moves the movable element **209** when activated as described in more detail below with reference to Figures 3A and 3B. The first SMA actuator **207** can be fabricated from any known material with shape memory characteristics, for example, nitinol. As known by those of skill in the art, SMAs can be fabricated to take on a predetermined shape when activated. In some embodiments, SMAs can be fabricated to expand or contract when activated from their deactivated state. In other embodiments, SMAs can be configured to expand or contract and rotate when activated from their deactivated state. Activation of a SMA actuator consists of heating the SMA such that it adopts its trained shape. In some embodiments, activation is accomplished by applying an electric current across the SMA element. Deactivation of a SMA actuator can be accomplished by turning off current to the SMA or otherwise cooling the SMA in order to allow the SMA to return to its pliable state as it cools. In some embodiments, there are electrical contacts and an insulated area in the local actuator **103** which allow activation of the first SMA actuator **207**. Activation of the first SMA actuator **207** to its trained shape results in a force which can be utilized by the local actuator **103** to move the movable element **209** in a first direction, for example, along an axis between the first element **205** and the second element **213**.

[0032] As one of skill in the art will recognize, SMA actuators can take numerous shapes and configurations other than the helical shape of the first SMA actuator **207** shown in Figure 1. For example, a SMA is a straight wire, circular wire, or spiral wire. A SMA does not need to have a circular cross-section, for example, it can have a square, rectangular, polygonal, generally curvilinear, or irregularly shaped cross-section. In some embodiments, multiple SMA elements are coupled together to form a single SMA actuator **207**. Additionally, other types of actuators, for example, an electromagnetic motor, a solenoid, or piezoelectric actuator, can be used in place of a first SMA actuator **207** in the local actuator **103**. By alternatively activating and deactivating the first SMA actuator **207**, a cyclical movement of the moveable element **209** will result. This cyclical movement can be rotational about the longitudinal axis or back and forth along an axis that is generally and/or substantially parallel to the longitudinal axis.

[0033] The first SMA actuator **207** can be very small such that it has a width between about $5\mu\text{m}$ and about $1000\mu\text{m}$, with the preferred size being between about $5\mu\text{m}$ and about $100\mu\text{m}$. The first SMA actuator **207** preferably has a diameter that is, is about, is at least, is at least about, is not more than, is not more than about 5, 10, 20, 30, 40, 50, 60, 70, 80, 90, 100, 200, 300, 400, 500, 600, 700, 800, 900, or $1000\mu\text{m}$, or within a range defined by, and including, any two of these values. The range of lengths preferred for the first SMA actuator **207** in its relaxed or deactivated state ranges from about $20\mu\text{m}$ to about 10mm, with the preferred length being from about $200\mu\text{m}$ to about 10mm. The first SMA actuator **207** preferably has an overall length that is, is about, is at least, is at least about, is not more than, is not more than about 20, 30, 40, 50, 60, 70, 80, 90, 100, 200, 300, 400, 500, 600, 700, 800, 900 μm , 1, 2, 3, 4, 5, 6, 7, 8, 9, 10, 11, 12, 13, 14, 15, 16, 17, 18, 19, or 20 mm, or within a range defined by, and including, any two of these values.

[0034] In some embodiments, the second element **213** is connected or coupled with the movable element **209** by a biasing element **211**. The biasing element **211** can be made from materials which are not rigid, including elastic, superelastic, and non-elastic materials. In some embodiments, the biasing element **211** comprises a spring, for example, a tension spring or compression spring. In other embodiments, the biasing element **211** comprises a second SMA actuator configured to move between activated and deactivated states. The biasing element **211** can be formed from various materials, including elastic alloys, for example, Cu-Al-Ni, Cu-Al, Cu-Zn-Al, Ti-V, and Ti-Nb alloys.

[0035] The biasing element **211** can be very small such that it has a width between about $5\mu\text{m}$ and about $1000\mu\text{m}$, with the preferred size being between about $5\mu\text{m}$ and about $100\mu\text{m}$. The biasing element **211** preferably has a diameter or width that is, is about, is at least, is at least about, is not more than, is not more than about 5, 10, 20, 30, 40, 50, 60, 70, 80, 90, 100, 200, 300, 400, 500, 600, 700, 800, 900, or $1000\mu\text{m}$, or within a range defined by, and including, any two of these values. The range of lengths preferred for the biasing element **211** in its relaxed or deactivated state ranges from about $20\mu\text{m}$ to about 10mm, with the preferred length being from about $200\mu\text{m}$ to about 10mm. The biasing element **211** preferably has an overall length that is, is about, is at least, is at least about, is not more than, is not more than about 20, 30, 40, 50, 60, 70, 80, 90, 100, 200, 300, 400, 500, 600, 700, 800, 900 μm , 1, 2, 3, 4, 5, 6, 7, 8, 9, 10, 11, 12, 13, 14, 15, 16, 17, 18, 19, or 20 mm, or within a range defined by, and including, any two of these values.

[0036] The biasing element **211** is configured to apply a force to the movable element **209** that opposes the force applied by the first SMA actuator **207** on the movable element **209**. This opposing force can move the movable element **209** in a direction counter to the direction the movable element **209** moves when the first SMA actuator is activated. The movement of the movable element **209** can be appreciated by comparing Figures 2A and 2B. In Figure 2A, the movable element **209** is in a first position (e.g., closer to the second element **213** than the first element **205**). In Figure 2B, the movable element **209** is in a second position (e.g., closer to the first element **205** than the second element **213**).

[0037] In an alternative embodiment, one or both of the first and second elements **205**, **213** are eliminated and one end of the first SMA actuator **207** and/or the biasing element **211** are secured directly to the elongated body **101** or housing **215**. In another alternative embodiment, one or both of the first and second elements **205**, **213** are secured

indirectly to the elongated body **101** through an intermediate element, for example, a housing **215** for the local actuator **103**. In some embodiments, the first SMA actuator **207** is coupled with the movable element **209** and the second element **213**, and the biasing element **211** is coupled with the movable element **209** and the first element **213**. In another embodiment, the local actuator **103** comprises only a first element **205**, a movable element **209**, and a single SMA actuator **207** coupled with the movable element **209** and the first element **205**. The single SMA actuator **207** moves the movable element **209** in a first direction when actuated.

[0038] Figures 2C-2E show embodiments of a local actuator **103** where a first SMA actuator **207** and biasing element **211** are configured in parallel to one another. The first SMA actuator **207** is connected to a first element **205** that is secured to and preferably does not move relative to an elongated body **101**. The other end of the first SMA actuator **207** is coupled with a movable element **209**. Similarly, a biasing element **211** is coupled with the first element **205** and the movable element **209**. The biasing element **211** can comprise any deformable component, for example, a spring or second SMA actuator, and can be configured to apply a force on the movable element **209** that is counter to the force applied on the movable element by the SMA actuator **207** when the first SMA actuator **207** is activated. In Figure 2C, the movable element **209** is disposed between the cam **201** and the first element **205**. In Figure 2D, the first element **205** is disposed between the movable element **209** and the cam **201**. In Figure 2E, the SMA actuator **207** and the biasing element **211** are disposed concentrically around the shaft **203**. Thus, one of skill in the art will recognize that a first SMA actuator can optionally be paired with another biasing element **211** in parallel or series to produce a linear oscillating motion for a connected movable element **209**.

[0039] As shown in the embodiments in Figures 2A - 2E, the movable element **209** is connected to or comprises an arm or shaft **203** such that movement of the movable element **209** results in movement of the shaft **203**. The shaft **203** can extend from the movable element **209** towards the distal end of the elongated body **101**. In some embodiments, the shaft **203** can optionally extend from the movable element **209** towards the proximal end of the elongated body **101**. The first element **205** and second element **213** optionally include openings to allow at least a portion of the shaft **203** to pass through the first and/or the second elements. One of skill in the art will recognize that the shaft **203** can be offset such that it does not have to pass through the first or second elements **205**, **213** in order to extend through or move past these elements. For example, a portion of the shaft **203** can extend laterally from the movable element **209** and then turn and extend along an axis that is generally parallel to the longitudinal axis. In some embodiments, the shaft **203** itself can be used in place of a movable element **209** by directly connecting the SMA actuator **207** to the shaft **203**. In other embodiments, the movable element **209** and shaft **203** are an integral component.

[0040] A distal end of the shaft **203** is coupled to or comprises a cam **201** that is configured to move along with the movable element **209** and the shaft **203** as the first SMA actuator **207** is alternated between an activated and a deactivated state. The cam **201** is configured to engage, for example, contact, pull, or push, another object. In some embodiments, the cam **201** is configured to engage an ultrasound transducer element in order to move the ultrasound transducer element between at least a primary position and a secondary position as the movable element **209** moves back and forth between two positions. In some embodiments, the cam **201** is configured to engage an ultrasound transducer element in order to rotate the ultrasound transducer element between at least a primary position and a secondary position as the movable element **209** linearly moves back and forth between a first position and a second position. In other embodiments the shaft **203** directly contacts an ultrasound transducer element. In some embodiments, the movable element **209**, shaft **203**, and cam **201** are a single movable piece. In other embodiments, the movable element **209**, shaft **203**, and cam **201** are each separate pieces connected to one another. In one embodiment, a simple pin joint is disposed between the shaft **203** and an ultrasound transducer element. The pin joint, or similar structure, is configured to convert linear motion into rotational motion.

[0041] The cam **201**, shaft **203**, and movable element **209** can be connected in various configurations. In some embodiments, the shaft **203** comprises more than one piece or member that move relative to one another. For example, in one embodiment, the shaft **203** comprises a first link that is pivotally connected to the movable element **209** and a second link that is pivotally connected to the first link and the cam **201**. In some embodiments, the shaft **203** extends in a direction that is not substantially parallel to the longitudinal axis or has a portion that extends in a direction that is generally normal to the longitudinal axis. In some embodiments, the shaft **203** may be pivotally connected to the movable element **209** and/or the cam **201**. In some embodiments, the shaft **203** moves relative to the movable element **209** and/or the cam **201**. In some embodiments, the cam **201** may move, flex, or deflect, relative to the shaft **203** and/or movable element **209**. In some embodiments, the cam **201** is pivotally connected to the shaft **203**. In other embodiments, the cam **201** comprises a flexible material.

[0042] Figures 3A and 3B are diagrams showing how the motion of a SMA actuator comprised of nitinol is controlled. For the sake of simplicity, Figure 3A shows how the rotational motion of a SMA shaft is controlled and Figure 3B shows how the longitudinal motion of a SMA shaft is controlled. However, one can combine the configurations illustrated in the two diagrams to achieve both rotational and longitudinal motion simultaneously.

[0043] Figure 3A shows an SMA actuator **207** in a Martensite State and the same SMA actuator **207** in an Austenite State. The SMA actuator **207** is helically shaped. In the Martensite State, the SMA actuator **207** has a pitch (e.g., the

height of one full turn) defined as h_1 , a radius defined as r_1 , and the length of the wire making one complete rotation is defined as L_1 . In the Austenite State, the SMA actuator 207 has a pitch defined as h_2 and a radius defined as r_2 , and the length of the wire making one complete rotation is defined as L_1 . The relationship between the helix radius, pitch, and wire length is defined by the Pythagorean Theorem as:

$$(h_1)^2 + (2\pi r_1)^2 = (L_1)^2 \quad \text{[Equation 1]}$$

and

$$(h_2)^2 + (2\pi r_2)^2 = (L_2)^2 \quad \text{[Equation 2]}$$

[0044] Ignoring any contraction effects, the length of the wire wrapped into the helix remains the same regardless of the helical shape that it forms. To simplify, an assumption can be made that the wire makes one complete helical turn in the austenite state. Therefore,

$$(h_1)^2 + (2\pi r_1)^2 = (L_1)^2 \quad \text{[Equation 3]}$$

and

$$n(h_1) = h_2 \quad \text{[Equation 4]}$$

wherein n is the number of turns the helix makes around in the Martensite State. By substituting equations 3 and 4 into equations 1 and 2 and solving for n, we are left with the following relationship:

$$n = \frac{r_2}{r_1} \quad \text{[Equation 5]}$$

[0045] This relationship indicates that the maximum achievable rotation is defined by the ratio of the radii in the Austenite State and the Martensite State. A partial transformation of the nitinol SMA actuator 207 from the lower temperature Martensite State to the high temperature Austenite State will result in a proportional reduction in achieved rotation. One can choose the desired level of rotation by selecting the appropriate ratio between the two radii.

[0046] Figure 3B shows a SMA actuator 207 in a Martensite State and an Austenite State. In the Martensite State, the SMA actuator 207 has a pitch (e.g., the height of one full turn) defined as h_1 and a radius defined as r_1 , the length of the wire making one complete rotation is defined as L_1 , and the number of helical turns is defined as n_1 . In the Austenite State, the SMA actuator 207 has a pitch defined as h_2 and a radius defined as r_2 , the length of the wire making one complete rotation is defined as L_1 , and the number of helical turns is defined as n_2 . The relationship between the helix radius, pitch, and wire length is defined by the Pythagorean Theorem disclosed in equations 1 and 2. The longitudinal motion of the SMA actuator 207 between the Martensite State and Austenite State can be determined by the following equation:

$$\text{Longitudinal motion} = (n_1)(h_1) - (n_2)(h_2) \quad \text{[Equation 6]}$$

[0047] Figure 4A shows an embodiment of an ultrasound transducer element 105 that includes a transducer 401, a transducer mount 405, a coupling member 111, and an electrical wire 409. The transducer 401 includes at least one ultrasound transducer crystal configured to send and receive ultrasound signals and the transducer 401 is preferably mounted on a backing 403. The transducer 401 can have various shapes, for example, square or cylindrical. In some embodiments, the transducer 401 is directly coupled with a transducer mount 405. The shape and size of the transducer mount 405 can vary depending on the shape and size of the transducer 401 or backing 403, to be coupled with the mount 405. In some embodiments, the transducer mount 405 is ring shaped with an aperture through the mount 405. In some embodiments, the transducer mount 405 includes a recess or indentation configured to receive at least a portion of a cam when the cam is engaged with the transducer mount.

[0048] The transducer mount 405 can optionally include a push bar 406 configured to engage a cam 201. The push

bar **406** can be a pin, bar, cylinder, or similar structure that extends from the body of the transducer mount **405** to provide a point of contact for a cam **201**. In some embodiments, the cam **201** engages one general side of the push bar **406** and in other embodiments, the cam **201** engages more than one side or portion of the push bar **406**. In some embodiments, the cam **201** is fixed to the push bar **406** or transducer **405** and in other embodiments, the cam **201** is not fixed to the push bar **406**.

[0049] In some embodiments, the transducer **401** can be made to have a thickness or length that is between about $5\mu\text{m}$ and about $1500\mu\text{m}$, with a preferred size being between about $5\mu\text{m}$ and about $1000\mu\text{m}$, or more preferably between about $200\mu\text{m}$ and about $700\mu\text{m}$. The transducer **401** preferably has a thickness or length that is, is about, is at least, is at least about, is not more than, is not more than about 5, 10, 20, 30, 40, 50, 60, 70, 80, 90, 100, 200, 300, 400, 500, 600, 700, 800, 900, 1000, 1100, 1200, 1300, 1400 or 1500, μm or within a range defined by, and including, any two of these values.

[0050] In the illustrated embodiment, the transducer mount **405** has or is coupled with a coupling member **111** such that the transducer mount and transducer **401** are configured to rotate about the coupling member. In other embodiments, the transducer mount **405** and/or transducer **401** are directly coupled with an elongated body or other fixed object and configured to rotate about an axis of rotation relative to the elongated body or other fixed object. The coupling member **111** can have various shapes and sizes depending on the transducer mount **405** and/or the transducer **401**. For example, the coupling member **111** can include a cylindrical pin, cylindrical dowel, or differently shaped member. In other embodiments, the transducer mount **405** and/or transducer **401** are configured to rotate about a different revolute joint, for example, a cylindrical joint, a screw joint, or a ball and socket joint. For example, a transducer mount **405** may include a ball and the elongated body **101** may include a socket configured to receive at least a portion of the ball to facilitate rotation of the transducer mount **405** relative to the elongated body **101**. In another example, the transducer mount **405** may include one or more pins configured to rotate relative to one or more openings or sockets in the elongated body **101**. Alternatively, the transducer mount **405** has a socket or opening for a ball or pin disposed on the elongated body **101**. In some embodiments, the ultrasound transducer element **105** is configured to rotate around an axis of rotation that is substantially normal to the longitudinal axis. In some embodiments, the ultrasound transducer element **105** is configured to rotate around an axis of rotation that is not substantially normal to the longitudinal axis. In one embodiment, the axis of rotation of the ultrasound transducer element **105** may form about a 45 degree angle with the longitudinal axis.

[0051] In some embodiments, the electrical wire **409** is connected to the transducer **401**. For example, in one embodiment, the electrical wire **409** is connected to the proximal surface of the transducer **401**. In another embodiment, multiple electrical wires, for example, two, are connected to two or more surfaces of the transducer **401**. The wire **409** can be the same as wire **109** in Figure 1. The wire **409** can connect the transducer **401** with an electrical cable, for example, a coaxial or twisted pair, that is connected to an imaging system. In some embodiments, a wireless transmitter (not shown) is used to connect the transducer **401** to an imaging system. In some embodiments, the transducer mount **405** acts as an electrical conductor. In an embodiment, electrical wires **409** are coupled to the transducer **401** through non-contact coupling (e.g., capacitive or inductive coupling) which is commonly used in conventional intravascular imaging systems.

[0052] The electrical wire **109** can have various shapes and sizes. For example, the electrical wire **109** can have a generally circular cross-section with a diameter of about $100\mu\text{m}$. The electrical wire **109** preferably has a diameter that is, is about, is at least, is at least about, is not more than, is not more than about 1, 2, 3, 4, 5, 6, 7, 8, 9, 10, 20, 30, 40, 50, 60, 70, 80, 90, or $100\mu\text{m}$, or within a range defined by, and including, any two of these values.

[0053] In some embodiments, the electrical wire **409** is wrapped at least partially around the coupling member **111** or other portion of the transducer mount **405** such that it acts to bias the transducer **401** and transducer mount **405** in a certain direction. In one embodiment, the electrical wire **409** forms a coil around the coupling member **111** that acts as a mechanical spring that stores elastic energy as the transducer **401** rotates in a first direction and applies the energy to bias the transducer **401** in a direction counter to the first direction. Thus, the electrical wire **409** can be used to return the transducer mount **405** and transducer **401** to a primary position after the transducer mount and transducer **401** have rotated or moved away from the primary position to a secondary position. Utilizing the electrical wire **409** as a biasing force eliminates the need for additional force or resistance for the scanning motion resulting in a device **100** that is more efficient (e.g., requires less energy) and has a longer scanning time producing better imaging quality. In embodiments where an electrical wire **409** or other structure applies a biasing force on the transducer mount **405**, the device **100** requires less energy to operate. One of skill in the art will understand that a spring or similar biasing structure that is not an electrical wire coiled around the coupling member **111** can also be used to bias the transducer mount **405** and transducer **401** towards a certain direction or position.

[0054] In a preferred embodiment, the ultrasound transducer element **105** rotates about an axis of rotation as another object, for example, a cam, applies a linear force on the transducer mount **405**. In some embodiments, the ultrasound transducer element **105** continues to rotate after a force is applied on the transducer mount due to the moment of inertia of the transducer **401** and/or transducer mount **405**. Generally, the higher moment of inertia is, the more the ultrasound transducer element **105** will continue to rotate after a linear force is applied to the transducer mount **405**. The moment of inertia is mostly determined by the center of mass of the rotating body and the distance between the center of mass

and the axis of rotation. Thus, the moment of inertia of the rotating portions of the ultrasound transducer element **105** can be adjusted by adjusting the mass, size, and location of the rotating portions. For example, a longer transducer element **401** is used to increase distance from the center of mass of the transducer element **401** and the axis of rotation.

[0055] The size of the ultrasound transducer element **105** itself contributes largely to the overall ultrasound device **100** size, so it is important that a smaller transducer **401** produces an image with quality that is comparable to a larger transducer **401**. Increasing the density of any backing layer **403** or transducer mount **405** can minimize the transducer length and overall ultrasound transducer element **105** size.

[0056] As shown in Figures 4A and 4B, in some embodiments, the moment of inertia of the rotating portions of the ultrasound transducer element **105** can be increased by adding a high density material layer **407**, optionally the same as the backing **403**. Figure 4B shows an embodiment of an ultrasound transducer element **105** with a high density material layer **407** added between the transducer **401** and the transducer mount **405**. The high density material layer **407** can comprise any high density material, for example, stainless steel, tungsten, gold, silver, platinum, copper, or titanium. Figure 4C shows another embodiment with a tubular high density material layer **407** that is placed around the transducer **401** to add mass to the rotating elements of the ultrasound transducer element **105**. In other embodiments, a combination of a high density backing layer **407** and tubular structure are used to increase the moment of inertia.

[0057] In some embodiments, the volume of the ultrasound transducer element **105** is about 0.1 cubic mm. In other embodiments, the volume of the ultrasound transducer element **105** is, is about, is at least, is at least about, is not more than, is not more than about 0.01, 0.02, 0.03, 0.04, 0.05, 0.06, 0.07, 0.08, 0.09, 0.1, 0.11, 0.12, 0.13, 0.14, 0.15, 0.16, 0.17, 0.18, 0.19, 0.2, 0.21, 0.22, 0.23, 0.24, 0.25, 0.26, 0.27, 0.28, 0.29, or 0.3 cubic mm. In some embodiments, the mass of the ultrasound transducer element **105** is about 1 mg. In other embodiments, the mass of the ultrasound transducer element **105** is, is about, is at least, is at least about, is not more than, is not more than about 0.2, 0.3, 0.4, 0.5, 0.6, 0.7, 0.8, 0.9, 1, 1.1, 1.2, 1.3, 1.4, 1.5, 1.6, 1.7, 1.8, 1.9, 1.8, or 2 mg, or within a range defined by, and including, any two of these values. In some embodiments, the ultrasound transducer element **105** may be generally cylindrical with a diameter or width that is, is about, is at least, is at least about, is not more than, is not more than about 0.4, 0.5, 0.6, 0.7, 0.8, 0.9, 1, 1.1, 1.2, 1.3, 1.4, 1.5, 1.6, 1.7, 1.8, 1.9, 2, 2.1, 2.2, 2.3, 2.4, 2.5, 2.6, 2.7, 2.8, 2.9, or 3 mm, or within a range defined by, and including, any two of these values. In some embodiments, the ultrasound transducer element **105** has a height that is, is about, is at least, is at least about, is not more than, is not more than about 0.1, 0.2, 0.3, 0.4, 0.5, 0.6, 0.7, 0.8, 0.9, 1, 1.1, 1.2, 1.3, 1.4, 1.5, 1.6, 1.7, 1.8, 1.9, 2, 2.1, 2.2, 2.3, 2.4, or 2.5 mm, or within a range defined by, and including, any two of these values.

[0058] Figure 5 shows an embodiment of an intravascular ultrasound device **100** including a local actuator **103** and an ultrasound transducer element **105** configured to rotate about an axis of rotation and a coupling member **111** relative to the elongated body **101**. The cam **201** of the local actuator **103** is configured to move in a first linear direction and a second linear direction that is counter to the first linear direction along with the movable element **209** (not shown). In some embodiments, when moving in a linear direction, the cam **201** engages the transducer mount **405** at the push bar **406** and causes the ultrasound transducer element **105** to rotate about the axis of rotation in a first direction.

[0059] In general, the first SMA actuator **207** is used to generate a large linear displacement which has intrinsic limitations on how fast it moves and how much power it requires. In some embodiments, because of geometric constraints (e.g., the dimensions of a vasculature) the cam **201** can collide with the transducer mount **405** other than at the push bar **406** when moving in first a linear direction causing the cam **201** to stop moving in the first linear direction and causing the ultrasound transducer element **105** to stop rotating before the desired amount of rotation of the transducer element **105** is achieved. For example, if the cam **201** is configured to push the transducer mount **405** to cause the ultrasound transducer element **105** to rotate, it works fine within a certain angle of rotation (e.g., less than about 60°) but is limited when pushing farther to cause a larger angle of rotation (e.g., up to about 180°). In some embodiments, when the cam **201** pushes on the push bar **406** for longer distances, the cam **201** starts colliding with the transducer mount **405** and the rotation of the ultrasound transducer element **105** is stopped prematurely.

[0060] The problem of the cam **201** colliding with the transducer mount **405** where not desired can be addressed by configuring the local actuator **103** to apply an amplified force or impulse force to the ultrasound transducer element **105**. Applying an impulse force to the ultrasound transducer element **105** utilizes the moment of inertia of the ultrasound transducer element **105** to rotate the ultrasound transducer element **105** about the axis of rotation after the cam **201** and the push bar **406** portion of the transducer mount have disengaged from one another. In one embodiment, the cam **201** pushes the ultrasound transducer element **105** to a certain point and the transducer element **105** continues to rotate beyond where the cam **201** stops because of the moment of inertia. In embodiments where the ultrasound transducer element **105** includes an electrical wire **109**, or other elastic element, configured to bias the ultrasound transducer element **105** in a certain direction counter to the direction of rotation caused by the impulse force, the ultrasound transducer element **105** will return back to a primary position or origin due to the applied biasing force. In some embodiments, the biasing element **211** in the local actuator **103** is optionally omitted and the electrical wire **409**, or other biasing element in the transducer element **105**, returns the cam **201** and movable element **209** to the starting position as ultrasound transducer element **105** rotates to its starting or primary position.

[0061] Turning now to Figures 6A - 6C, an embodiment of an intravascular ultrasound device **100** including a local actuator **103** configured to apply an upward force on the transducer mount **405** is shown. Figure 6A shows the cam **201** and the transducer mount **405** initially engaged in a primary position. The first SMA actuator **207** is activated to move the movable element **209** towards the distal end of the elongated body **101**. The shaft **203** and cam **201** move along with the movable element **209** and engage the transducer mount **405** and push bar **406**. The transducer mount **405** begins to rotate counter-clockwise while the cam **201** continues to move towards the distal end. In another embodiment, if the moment of inertia of the transducer element **105** is high enough, the shaft **203** can directly push the transducer mount **405**, or the ultrasound transducer element **105**, and a cam **201** is not necessary to achieve the leverage in the scanning motion.

[0062] Figure 6B shows an example of a point where the movable element **209**, shaft **203**, and cam **201** stop moving towards the distal end and the cam **201** and transducer mount **405** disengage from one another. At this point, the first SMA actuator **207** is preferably deactivated and the biasing element **211** causes the movable element **209**, shaft **203**, and cam **201** to move in the opposite direction (e.g., towards the position in Figure 6A). Even though the cam **201** and transducer mount **405** disengage at this point, the ultrasound transducer element **105** preferably continues to rotate counter-clockwise about the axis of rotation and coupling member **111**. The ultrasound transducer element **105** may continue to rotate about the axis of rotation after disengagement from the cam **201** because of the moment of inertia of the ultrasound transducer element **105**. The transducer element **105** may also include an optional biasing element that assists the continued rotation of the transducer element **105** in the counter-clockwise direction after the transducer mount **405** disengages from the cam **201**. For example, the ultrasound transducer element **105** may include a spring configured to bias the transducer element to rotate counter-clockwise about the axis of rotation of the coupling member **111**.

[0063] As shown in Figure 6C, the ultrasound transducer element **105** can continue to rotate counter-clockwise to a secondary position where the electrical wire **109** or similar structure biases the ultrasound transducer element **105** to rotate in a counter direction (e.g., clockwise) back towards its origin or primary position. The biasing element **211** will move the movable element **209**, shaft **203**, and cam **201** back to their initial or primary position (e.g., the position in Figure 6A) and the ultrasound transducer element **105** can continue rotating until it contacts the cam **201** in the first position or until it reaches some other equilibrium. Thus, the oscillating linear movement of the movable element **209**, shaft **203**, and cam **201** can be used to rotate the ultrasound transducer element **105** back and forth about an axis of rotation to create a forward-looking sweeping motion of the transducer **401**. In another embodiment, one or more mechanical stops (not shown) are included to further limit the rotation of the ultrasound transducer **105**.

[0064] The device **100** can be configured for side-looking as well as forward-looking, for example, by placing an ultrasound transducer element **105** or a reflective surface (not shown) such as a mirror in different configurations. In some embodiments, the angle of orientation of the ultrasound transducer element **105** or mirror relative to the longitudinal axis of the device **100** is any angle between about 15° and about 165°, with the preferred angle for side-looking device **100** being between about 80° and about 110°. Angles contemplated include about 15, 20, 25, 30, 35, 40, 45, 50, 55, 60, 65, 70, 75, 80, 85, 90, 95, 100, 105, 110, 115, 120, 125, 130, 135, 140, 145, 150, 155, 160, and about 165 degrees, or within a range defined by, and including, any two of these values.

[0065] The range of motion generated by the local actuator **103** described herein will vary depending of the application. Rotational motion of the transducer element can oscillate in a range from about 1 or 2 degrees up to about 270 degrees. The angle of rotational displacement that can be generated by the local actuator **103** is, is about, is at least, is at least about, is no more than, or is no more than about, 1, 2, 5, 10, 15, 20, 25, 30, 35, 40, 45, 50, 55, 60, 65, 70, 75, 80, 85, 90, 95, 100, 105, 110, 115, 120, 125, 130, 135, 140, 145, 150, 155, 160, 165, 170, 175, 180, 190, 200, 210, 220, 230, 240, 250, 260, or 270 degrees, or within a range defined by, and including, any two of these values. In a preferred embodiment the transducer **401** scans an equivalent direction to either side of the longitudinal axis, such that the device **100** is imaging directly in front of the distal tip of the device. Also it is possible to amplify the angular displacement by simply utilizing different shapes of the transducer mount **405**, especially where it has an interaction/contact with the cam **201**. In other embodiments, the scanning motion is directed to one side of the device, such that the imaging field is not symmetrical relative to the longitudinal axis. By adjusting the speed of scanning motion, the scanning rate can be adjusted while the device is in the patient, allowing the operator to adjustably define a specific frame rate in real-time images. The preferred range of rotational displacement or angle of rotation generated by the device **103** is from about 30 to 180 degrees. In addition, it is possible to use the device **100** for single point interrogation for optical coherence reflectometry or Doppler Effect measurements.

[0066] Figures 7A - 7D show another embodiment of an intravascular ultrasound device **100** where the first SMA actuator **207** is configured to expand and push the movable element **109** down (e.g., away from the distal end of the elongated body **101**) and the biasing element **211** is configured to move the movable element **209** and cam **201** towards the distal end. When the first SMA actuator **207** pushes the movable element **109** down, the shaft **203** moves with the movable element and pulls the cam **201** down as well. As the cam **201** moves down, the electrical wire **109** or other biasing force causes the ultrasound transducer element **105** to rotate clockwise, following the cam. In some embodiments the cam **201** and the transducer mount **405** can maintain engagement as the cam **201** moves down. In other embodiments,

the cam **201** and movable element **209** move faster than the ultrasound transducer element **105** resulting in disengagement between the cam **201** and the transducer mount **405**. The biasing element **211** is configured to move the movable element **209** and cam **201** back up to the first position shown in Figure 7A. As the biasing element **211** causes the cam **201** to move towards the distal end to its starting position, the cam **201** and transducer mount **405** is engaged, or re-engaged, causing the ultrasound transducer element **105** to rotate counter-clockwise and return to its primary or starting position (e.g., the position shown in 7A). In another embodiment, the cam **201** is configured to pull the transducer mount **405** down, optionally releasing the transducer mount **405** at a certain point. The electrical wire **409** or biasing force then causes the ultrasound transducer element **105** to rotate in a counter direction back to its primary position or origin.

[0067] Figures 8A and 8B show an embodiment where the cam **201** pulls instead of pushing the push bar **406**. Figure 8A shows the cam **201** and push bar **406** initially engaged in a primary position. The first SMA actuator **207** is activated to move the movable element **209** away from the distal end of the elongated body **101** pulling the push bar **406** and causing the ultrasound transducer element **105** to rotate clockwise towards a secondary position.

[0068] Figure 8B shows the ultrasound transducer element **105** in the secondary position. The ultrasound transducer element **105** can include a biasing element, for example, a coiled electrical wire **409** or spring (not shown), configured to bias the ultrasound transducer element **105** towards the primary position. In some embodiments, the linear actuator **103** does not require a biasing element or second SMA actuator **211** to return the cam **201** to the primary position because the biasing element in the ultrasound transducer element **105** pulls the cam **201** back to the primary position when the first SMA actuator **207** is deactivated. In some embodiments, the local actuator **103** includes a biasing element **211** such that the cam **201** pushes and pulls the transducer mount **405** in opposite directions resulting in a sweeping rotation movement of the ultrasound transducer **105**.

[0069] It is desirable to provide quality imaging for a physician to interpret accurately during an intervention. There are different ways to improve and achieve higher quality imaging. One way is to have a smooth and consistent scanning motion. Another way is to acquire as much data as possible and process the data through averaging and filtering in order to enhance different characteristics, for example, the signal to noise ratio. Thus, image quality can be enhanced by providing a consistent scanning motion and adjusting the time the scanning motion takes. To achieve an ideal scanning motion, an actuator drive waveform can be optimized to produce a consistent motion while maximizing the scanning time to acquire as much data as possible.

[0070] Figure 9A shows different examples of contemplated waveforms that can lead to different scanning motions. The wave forms are expressed as voltage versus time. Figure 9B shows how an active heating path and cooling path affect rotation of an ultrasound transducer element. Figure 9B shows the angle of rotation versus time for an active (heating) path and returning (cooling path).

[0071] The ultrasound device **100** must be able to operate for a certain period of time when used in invasive procedures. Depending on the type of intervention, the procedure could take a couple of hours or more and the ultrasound device **100** could be required to undergo about one million or more cycles of scanning. In general, SMA actuators are considered to have low fatigue properties and so it is critical, yet challenging, to achieve the required life cycle with a frame rate of 10Hz or higher as an imaging device. SMA actuators are able to continuously operate in millions of cycles so long as they do not undergo a large displacement or strain. The main challenge to achieving a large scanning motion required for clinically vital imaging is to balance the displacement of the SMA actuator with the fatigue properties of the SMA. For example, typically, a large scanning motion requires a large displacement of an SMA actuator resulting in diminished longevity of the SMA due to fatigue failure. However, the motion amplification disclosed in a preferred embodiment herein makes it feasible and practical to meet both the displacement and fatigue requirements simultaneously. In some embodiments, because of the motion amplification, the SMA actuator **207** only needs to produce a small displacement and therefore, undergoes less strain while the ultrasound transducer element **105** undergoes a large scanning motion. Thus, embodiments disclosed herein can be used for relatively long periods of time while still meeting the requirements of functional imaging devices used in invasive medical procedures.

[0072] In some embodiments of an ultrasound device **100**, it is desirable to provide real time imaging without losing valuable information during intervention. For real time imaging, certain frame rates are preferred depending on where to image. For example, for heart imaging, it is preferable to image a moving heart in a frame rate of 20Hz or higher considering how fast it is moving. Conventionally it becomes challenging to drive the first SMA actuator **207** higher than 10Hz because it requires enough cooling time to provide a practically functional motion. However, by utilizing the leverage present in preferred embodiments disclosed herein, it is possible to achieve a higher frame rate for imaging because the scanning motion is not largely determined by the first SMA actuator **207** itself. Also, to be able to drive the first SMA actuator **207** 10Hz or higher, the first SMA actuator **207** is typically in contact with water or other liquid that provides fast cooling. But embodiments disclosed herein make it possible to drive the first SMA actuator **207** at a frequency that is, is about, is at least, is at least about, is not more than, is not more than about 10Hz, 15Hz, 20Hz, 25Hz, 30Hz or within a range defined by, and including, any two of these values. This makes the manufacturing process for the device simpler and easier as a commercial product because there is no need to seal or fill a device with water or other liquid during assembly and packaging. By driving the first SMA actuator **207** in air, it requires less energy and demands less power

from an imaging system.

[0073] The first SMA actuator **207** is preferably surrounded by air. Air is a good insulator by itself, so it contributes to a lower operating temperature for the device **100** (e.g. the external temperature of the device while operating is, is about, is at least, is at least about, is not more than, is not more than about 25, 30, 35, 40, 43, 45, 50, 55, 60, 65, 70 degrees Celsius or within a range defined by, and including, any two of these values) which is more favorable considering possible negative effects on tissue when operating at high temperatures. In some embodiments, an optional housing **215** surrounding the first SMA actuator **207** (e.g. shown in Figure 2A) is made of an insulating material that further heat insulates the first SMA actuator **207** from the rest of the device **100**. Also, air makes the first SMA actuator **207** less susceptible to the surrounding environment, so it can produce consistent scanning motion regardless of blood flow, tissue, and body temperature.

[0074] The local actuator **103** can generate rotational displacement in a range from about 1Hz to about 50Hz. The preferred frequency of motion is between about 8Hz and 30Hz. The frequency of movement generated by the local actuator **103** is, is about, is at least, is at least about, is not more than, is not more than about 1, 2, 3, 4, 5, 6, 7, 8, 9, 10, 11, 12, 13, 14, 15, 16, 17, 18, 19, 20, 25, 30, 35, 40, 45, or 50 Hz, or within a range defined by, and including, any two of these values.

[0075] The first SMA actuator **207** can preferably be activated at various speeds, depending on the frame rate. Preferably, the first SMA actuator **207** is activated at between 0.1mSec and 50mSec. It is contemplated that the first SMA actuator **207** is preferably activated at a time constant that is, is about, is at least, is at least about, is not more than, is not more than about 0.1, 0.2, 0.3, 0.4, 0.5, 0.6, 0.7, 0.8, 0.9, 1, 2, 3, 4, 5, 6, 7, 8, 9, 10, 11, 12, 13, 14, 15, 16, 17, 18, 19, 20, 21, 22, 23, 24, 25, 26, 27, 28, 29, 30, 31, 32, 33, 34, 35, 36, 37, 38, 39, 40, 41, 42, 43, 44, 45, 46, 47, 48, 49, or 50 mSec, or within a range defined by, and including, any two of these values.

[0076] As shown in Figures 10A-10C, the intravascular ultrasound device **100** disclosed herein can be implemented in various medical devices **901**, for example, but not limited to, devices for stent placement and deployment, balloon angioplasty, directional atherectomy, cardiac ablation, PFO (patent foramen ovale) closure, transvascular re-entry, trans-septal punch, and CTO (chronic total occlusion) crossing. In another embodiment, the intravascular ultrasound device **100** can have a lumen or opening along the longitudinal axis configured to introduce a guide wire or other interventional devices, and provide real-time or nearly real-time guidance in front of or around the device. Another embodiment of the invention is a method of visualizing the interior of an organ or tissue having a lumen or cavity using the device described above.

[0077] For real-time imaging guidance, it is desirable to have a localized steering in the distal end of the device **100**. In a preferred embodiment a localized steering portion can be incorporated near or around the distal imaging tip for efficient navigation. The local steering can be activated by one, two, three, four or more local actuators placed in the distal end, so it can be remotely controlled. Or the local steering can be achieved by simple pull wires (one, two, three, four or more) attached to or around the distal end that extends to the proximal end of the device, so it can be manually activated by hands. Depending on the number of local actuators and pull wires, it can have various motions with multiple degrees of freedom (one, two, three, four or more).

[0078] In some embodiments, the device **100** can provide intravascular ultrasound imaging in a small device such that it is easier to use in invasive procedures. Some medical devices incorporating the device **100** can have an outside diameter that is placed inside a patient's vasculature that is between about 2Fr and about 3.5Fr (about 0.6mm to about 1.2mm), although sizes as small as 1Fr (0.33mm) are also contemplated. For peripheral applications, the outside diameter of the portion of the medical device placed in the patient's vasculature can be as large as about 12Fr (4mm). Generally, it is contemplated that the outside diameter of any portion of the disclosed devices **100**, including the proximal and/or distal ends, the main body of the device, or the portion of the device designed to be placed inside the patient, is, is about, is not less than, is not less than about, is not more than, is not more than about 0.3, 0.4, 0.5, 0.6, 0.7, 0.8, 0.9, 1.0, 1.1, 1.2, 1.3, 1.4, 1.5, 1.6, 1.7, 1.8, 1.9, 2.0, 2.1, 2.2, 2.3, 2.4, 2.5, 2.6, 2.7, 2.8, 2.9, 3.0, 3.1, 3.2, 3.3, 3.4, 3.5, 3.6, 3.7, 3.8, 3.9, 4.0, 4.1, 4.2, 4.3, 4.4, 4.5, 4.6, 4.7, 4.8, 4.9, 5.0 mm, or within a range defined by, and including, any two of these values.

[0079] In another embodiment, the intravascular ultrasound device **100** is combined with Fractional Flow Reserve (FFR), so a single device has the capability of the ultrasound imaging and FFR. FFR is able to measure the intravascular blood pressure which helps in determining the severity of intravascular stenosis. By combining two methods in a guide wire, a single guide wire can provide more useful information to guide complex interventional procedures. In some embodiments, the same transducer **401** can be used to do ultrasound imaging as well as pressure measurement. In other embodiments, a separate sensor can be embedded to measure the intravascular pressure.

[0080] The embodiments described above are largely directed to ultrasound imaging. However, devices incorporating the scanning mechanism are not limited to cardiovascular applications, and it is contemplated that the device can be used in other settings, preferably medical procedures, where visualization of a small lumen or cavity is required.

[0081] Although the embodiments described herein have the imaging devices and scanning mechanism located in the distal end of the apparatus or other elongate member, one of skill in the art will recognize that the imaging devices can be placed anywhere along the length of the device. In another embodiment, the imaging devices disclosed herein

are integrated into the distal end of an device's rigid section that defines the distal tip of an apparatus.

[0082] The foregoing description details certain embodiments of the invention. It will be appreciated, however, that no matter how detailed the foregoing appears in text, the invention can be practiced in many ways. As is also stated above, it should be noted that the use of particular terminology when describing certain features or aspects of the invention should not be taken to imply that the terminology is being re-defined herein to be restricted to including any specific characteristics of the features or aspects of the invention with which that terminology is associated. The scope of the invention should therefore be construed in accordance with the appended claims and any equivalents thereof.

Claims

1. A forward-looking intravascular ultrasound device (100) comprising:

an elongated body (101) having a longitudinal axis, an interior surface, an exterior surface, a proximal end, and a distal end;
 an ultrasound transducer element (105) disposed at least partially in the distal end of the elongated body (101) and configured to rotate between at least a primary position and a secondary position about an axis of rotation that is normal to the longitudinal axis; and
 a local actuator (103) comprising a first element (205), wherein the first element (205) is secured to and does not move relative to the body (101);
 a movable element (209), wherein the movable element (209) is configured to move longitudinally substantially parallel to the longitudinal axis between at least a first position and a second position, wherein the movable element (209) is configured to engage the ultrasound transducer element (105) at least when the movable element (209) moves from the first position to the second position; and
 a first Shape Memory Alloy actuator (207) coupled to the first element (205) and the movable element (209), wherein the first Shape Memory Alloy actuator (207) is configured to switch between an activated and deactivated state, wherein the movable element (209) moves from the first position to the second position upon activation of the first Shape Memory Alloy actuator (207);
 wherein the ultrasound transducer element (105) rotates about the axis of rotation at least when the movable element (209) and ultrasound transducer element (105) are engaged and the movable element (209) moves from the first position to the second position;
characterized in that
 the movable element (209) and ultrasound transducer element (105) are not engaged after the movable element (209) reaches the second position and the ultrasound transducer (105) continues to rotate about the axis of rotation towards the secondary position.

2. The device of claim 1, further comprising a biasing element (211) coupled to the movable element (209) and the first element (205), wherein the biasing element (211) is configured to move the movable element (209) from the second position to the first position.

3. The device of claim 1, further comprising:

a second element (213), wherein the second element (213) is secured to and does not move relative to the body (101); and
 a biasing element (211) coupled to the second element (213) and the movable element (209), wherein the biasing element (211) is configured to move the movable element (209) from the second position to the first position.

4. The device of claim 3, wherein the first and second elements (205, 213) are disposed along an axis that is substantially parallel to the longitudinal axis.

5. The device of claim 3, wherein the first and second elements (205, 213) are disposed along an axis that is substantially normal to the longitudinal axis.

6. The device of claim 3, wherein the biasing element (211) comprises a second Shape Memory Alloy actuator (211), wherein the second Shape Memory Alloy actuator (211) has an activated and a deactivated state and when the second Shape Memory Alloy actuator (211) is activated it opposes motion of the movable element (209) from the first position to the second position.

7. The device of claim 6, wherein the movable element (209) is disposed between the first element and the second element (205, 213).

8. The device of claim 1, further comprising:

an electrical wire (409) connected to the ultrasound transducer element (105),
the electrical wire (409) being configured to bias the ultrasound transducer element (105) towards the primary position.

9. The device of claim 8, further comprising a member (111) coupled with the interior surface of the elongated body (101) at or near the distal end, wherein the ultrasound transducer element (105) is configured to rotate about the member (111) between at least the primary position and the secondary position.

10. The device of claim 9, wherein the electrical wire (109, 409) is coiled at least partially around the member (111).

11. The device of any one of claims 1-8, wherein the movable element (209) and ultrasound transducer element (105) are not continuously engaged while the movable element (209) moves from the second position to the first position.

12. The device of claim 1, wherein the first element (205) comprises an aperture, and the movable element (209) is disposed at least partly within the aperture.

13. The device of claim 1, wherein the movable element (209) comprises a cam (201) connected to a shaft (203).

Patentansprüche

1. Nach vorn weisende intravaskuläre Ultraschallvorrichtung (100), umfassend:

einen länglichen Körper (101) mit einer Längsachse, einer Innenfläche, einer Außenfläche, einem proximalen Ende und einem distalen Ende;

ein Ultraschallwandlerelement (105), das zumindest teilweise in dem distalen Ende des länglichen Körpers (101) angeordnet ist und konfiguriert ist, um sich zwischen mindestens einer primären Position und einer sekundären Position um eine Rotationsachse zu drehen, die senkrecht zu der Längsachse verläuft; und

ein lokales Betätigungselement (103) umfassend ein erstes Element (205), wobei das erste Element (205) an dem Körper (101) befestigt ist und sich nicht in Bezug darauf bewegt;

ein bewegliches Element (209), wobei das bewegliche Element (209) konfiguriert ist, um sich in Längsrichtung im Wesentlichen Parallel zu der Längsachse zwischen mindestens einer ersten Position und einer zweiten Position zu bewegen, wobei das bewegliche Element (209) konfiguriert ist, um mit dem Ultraschallwandlerelement (105) zumindest dann zusammenzuwirken, wenn sich das bewegliche Element (209) aus der ersten Position in die zweite Position bewegt; und

ein erstes Betätigungselement aus einer Formgedächtnislegierung (207), das mit dem ersten Element (205) und dem beweglichen Element (209) gekoppelt ist, wobei das erste Betätigungselement aus einer Formgedächtnislegierung (207) konfiguriert ist, um zwischen einem aktivierten und einem deaktivierten Zustand umzuschalten, wobei sich das bewegliche Element (209) bei Aktivierung des ersten Betätigungselements aus einer Formgedächtnislegierung (207) aus der ersten Position in die zweite Position bewegt;

wobei sich das Ultraschallwandlerelement (105) zumindest dann um die Rotationsachse dreht, wenn das bewegliche Element (209) und das Ultraschallwandlerelement (105) in Zusammenwirkung gebracht sind und sich das bewegliche Element (209) aus der ersten Position in die zweite Position bewegt;

dadurch gekennzeichnet, dass das bewegliche Element (209) und das Ultraschallwandlerelement (105) nicht in Zusammenwirkung sind, nachdem das bewegliche Element (209) die zweite Position erreicht hat und sich der Ultraschallwandler (105) weiterhin um die Rotationsachse auf die sekundäre Position zu dreht.

2. Vorrichtung nach Anspruch 1, ferner umfassend ein Vorspannelement (211), das mit dem beweglichen Element (209) und dem ersten Element (205) gekoppelt ist, wobei das Vorspannelement (211) konfiguriert ist, um das bewegliche Element (209) aus der zweiten Position in die erste Position zu bewegen.

3. Vorrichtung nach Anspruch 1, ferner umfassend:

ein zweites Element (213), wobei das zweite Element (213) an dem Körper (101) befestigt ist und sich nicht in Bezug auf diesen bewegt; und
ein Vorspannelement (211), das mit dem zweiten Element (213) und dem beweglichen Element (209) gekoppelt ist, wobei das Vorspannelement (211) konfiguriert ist, um das bewegliche Element (209) aus der zweiten Position in die erste Position zu bewegen.

4. Vorrichtung nach Anspruch 3, wobei das erste und das zweite Element (205, 213) entlang einer Achse angeordnet sind, die im Wesentlichen parallel zu der Längsachse verläuft.

5. Vorrichtung nach Anspruch 3, wobei das erste und das zweite Element (205, 213) entlang einer Achse angeordnet sind, die im Wesentlichen senkrecht zu der Längsachse verläuft.

6. Vorrichtung nach Anspruch 3, wobei das Vorspannelement (211) ein zweites Betätigungselement aus einer Formgedächtnislegierung (211) umfasst, wobei das zweite Betätigungselement aus einer Formgedächtnislegierung (211) einen aktivierten und einen deaktivierten Zustand hat und das zweite Betätigungselement aus einer Formgedächtnislegierung (211), wenn es aktiviert ist, der Bewegung des beweglichen Elements (209) aus der ersten Position in die zweite Position entgegensteht.

7. Vorrichtung nach Anspruch 6, wobei das bewegliche Element (209) zwischen dem ersten Element und dem zweiten Element (205, 213) angeordnet ist.

8. Vorrichtung nach Anspruch 1, ferner umfassend:

einen elektrischen Draht (409), der mit dem Ultraschallwandlerelement (105) verbunden ist, wobei der elektrische Draht (409) konfiguriert ist, um das Ultraschallwandlerelement (105) in Richtung der primären Position vorzuspannen.

9. Vorrichtung nach Anspruch 8, ferner umfassend ein mit der Innenfläche des länglichen Körpers (101) an oder nahe dem distalen Ende gekoppeltes Element (111), wobei das Ultraschallwandlerelement (105) konfiguriert ist, um sich um das Element (111) zwischen mindestens der primären Position und der sekundären Position zu drehen.

10. Vorrichtung nach Anspruch 9, wobei der elektrische Draht (109, 409) zumindest teilweise um das Element (111) gewickelt ist.

11. Vorrichtung nach einem der Ansprüche 1 bis 8, wobei das bewegliche Element (209) und das Ultraschallwandlerelement (105) nicht kontinuierlich in Zusammenwirkung sind, während sich das bewegliche Element (209) aus der zweiten Position in die erste Position bewegt.

12. Vorrichtung nach Anspruch 1, wobei das erste Element (205) eine Apertur umfasst und das bewegliche Element (209) zumindest teilweise in der Apertur angeordnet ist.

13. Vorrichtung nach Anspruch 1, wobei das bewegliche Element (209) eine mit einer Welle (203) verbundene Nocke (201) umfasst.

Revendications

1. Dispositif intravasculaire prospectif à ultrasons (100) comprenant :

un corps (101) allongé ayant un axe longitudinal, une surface intérieure, une surface extérieure, une extrémité proximale et une extrémité distale ;
un élément transducteur à ultrasons (105) disposé au moins partiellement dans l'extrémité distale du corps (101) allongé et configuré pour tourner entre au moins une position primaire et une position secondaire autour d'un axe de rotation qui est normal à l'axe longitudinal ; et
un actionneur local (103) comprenant un premier élément (205), dans lequel le premier élément (205) est fixé au corps (101) et ne se déplace pas par rapport à celui-ci ;
un élément mobile (209), dans lequel l'élément mobile (209) est configuré pour se déplacer de façon longitudinale sensiblement en parallèle à l'axe longitudinal entre au moins une première position et une seconde position,

dans lequel l'élément mobile (209) est configuré pour mettre en prise l'élément transducteur à ultrasons (105) au moins lorsque l'élément mobile (209) se déplace de la première position à la seconde position ; et un premier actionneur à Alliage à Mémoire de Forme (207) couplé au premier élément (205) et à l'élément mobile (209), dans lequel le premier actionneur à Alliage à Mémoire de Forme (207) est configuré pour commuter entre un état activé et un état désactivé, dans lequel l'élément mobile (209) se déplace de la première position à la seconde position lors de l'activation du premier actionneur à Alliage à Mémoire de Forme (207) ; dans lequel l'élément transducteur à ultrasons (105) tourne autour de l'axe de rotation au moins lorsque l'élément mobile (209) et l'élément transducteur à ultrasons (105) sont en prise et que l'élément mobile (209) se déplace de la première position à la seconde position ;

caractérisé en ce que

l'élément mobile (209) et l'élément transducteur à ultrasons (105) ne sont pas en prise après que l'élément mobile (209) atteint la seconde position et le transducteur à ultrasons (105) continue à tourner autour de l'axe de rotation vers la position secondaire.

2. Dispositif selon la revendication 1, comprenant en outre un élément de sollicitation (211) couplé à l'élément mobile (209) et au premier élément (205), dans lequel l'élément de sollicitation (211) est configuré pour déplacer l'élément mobile (209) de la seconde position à la première position.

3. Dispositif selon la revendication 1, comprenant en outre :

un second élément (213), dans lequel le second élément (213) est fixé au corps (101) et ne se déplace pas par rapport à celui-ci ; et
un élément de sollicitation (211) couplé au second élément (213) et à l'élément mobile (209), dans lequel l'élément de sollicitation (211) est configuré pour déplacer l'élément mobile (209) de la seconde position à la première position.

4. Dispositif selon la revendication 3, dans lequel les premier et second éléments (205, 213) sont disposés le long d'un axe qui est sensiblement parallèle à l'axe longitudinal.

5. Dispositif selon la revendication 3, dans lequel les premier et second éléments (205, 213) sont disposés le long d'un axe qui est sensiblement normal à l'axe longitudinal.

6. Dispositif selon la revendication 3, dans lequel l'élément de sollicitation (211) comprend un second actionneur à Alliage à Mémoire de Forme (211), dans lequel le second actionneur à Alliage à Mémoire de Forme (211) a un état activé et un état désactivé et lorsque le second actionneur à Alliage à Mémoire de Forme (211) est activé, il s'oppose au mouvement de l'élément mobile (209) de la première position à la seconde position.

7. Dispositif selon la revendication 6, dans lequel l'élément mobile (209) est disposé entre le premier élément et le second élément (205, 213).

8. Dispositif selon la revendication 1, comprenant en outre :

un fil électrique (409) relié à l'élément transducteur à ultrasons (105),
le fil électrique ((409) étant configuré pour solliciter l'élément transducteur à ultrasons (105) vers la position primaire.

9. Dispositif selon la revendication 8, comprenant en outre un élément (111) couplé à la surface intérieure du corps allongé (101) au niveau ou près de l'extrémité distale, dans lequel l'élément transducteur à ultrasons (105) est configuré pour tourner autour de l'élément (111) entre au moins la position primaire et la position secondaire.

10. Dispositif selon la revendication 9, dans lequel le fil électrique (109, 409) est enroulé au moins partiellement autour de l'élément (111).

11. Dispositif selon l'une quelconque des revendications 1 à 8, dans lequel l'élément mobile (209) et l'élément transducteur à ultrasons (105) ne sont pas continuellement en prise tandis que l'élément mobile (209) se déplace de la seconde position à la première position.

12. Dispositif selon la revendication 1, dans lequel le premier élément (205) comprend une ouverture, et l'élément mobile

(209) est disposé au moins en partie à l'intérieur de l'ouverture.

- 13.** Dispositif selon la revendication 1, dans lequel l'élément mobile (209) comprend une came (201) reliée à un arbre (203).

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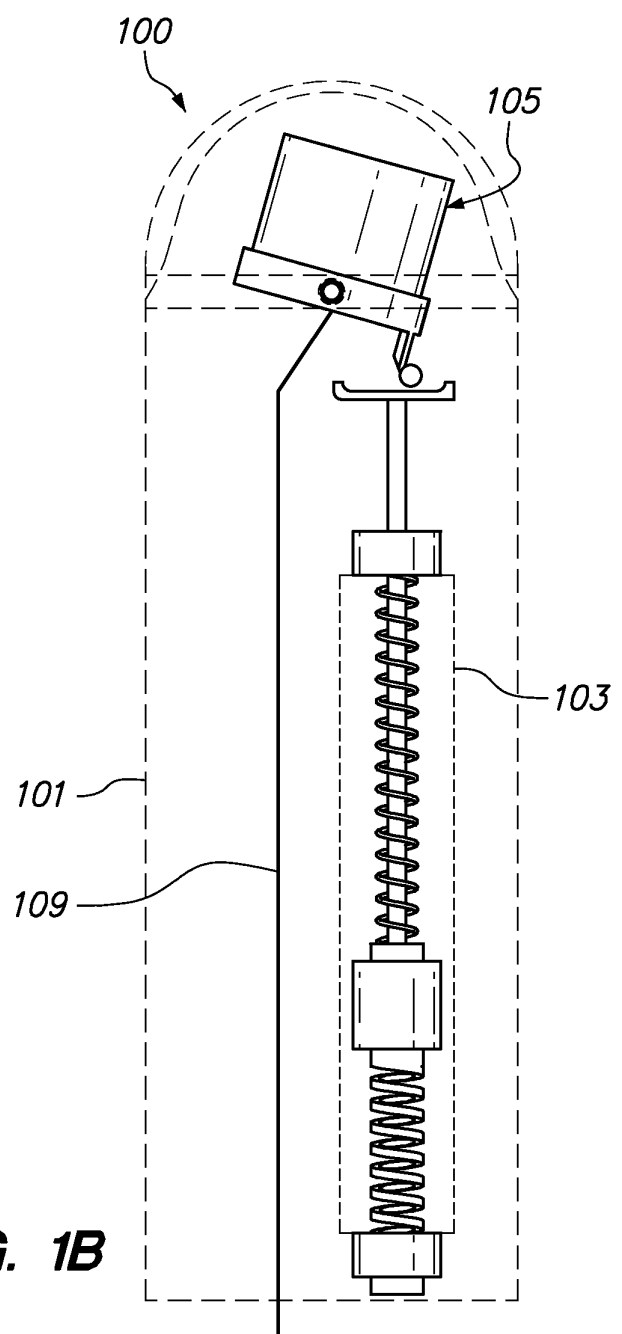
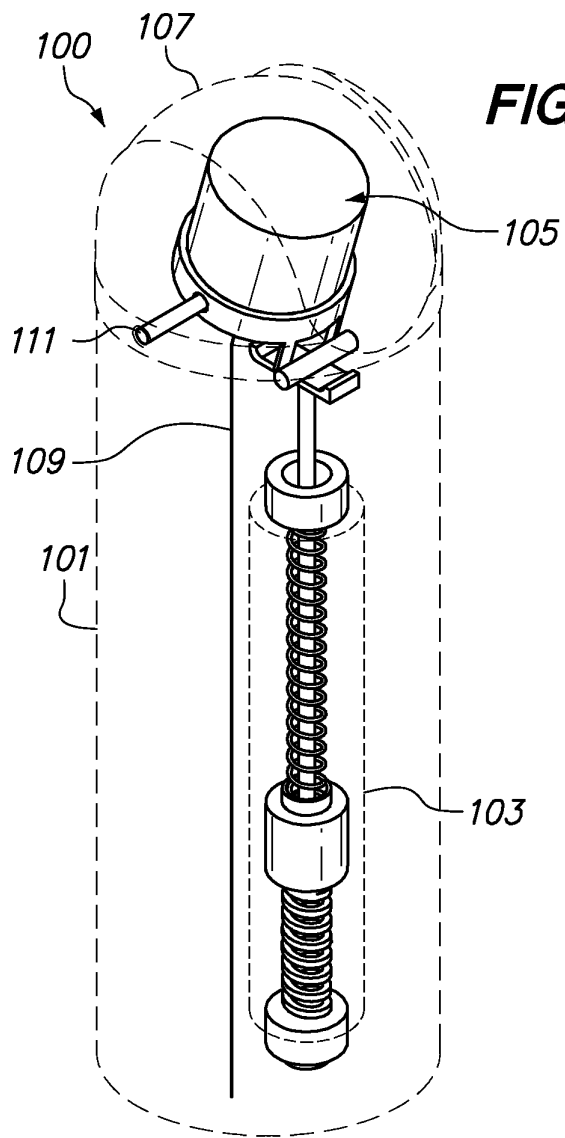


FIG. 2A

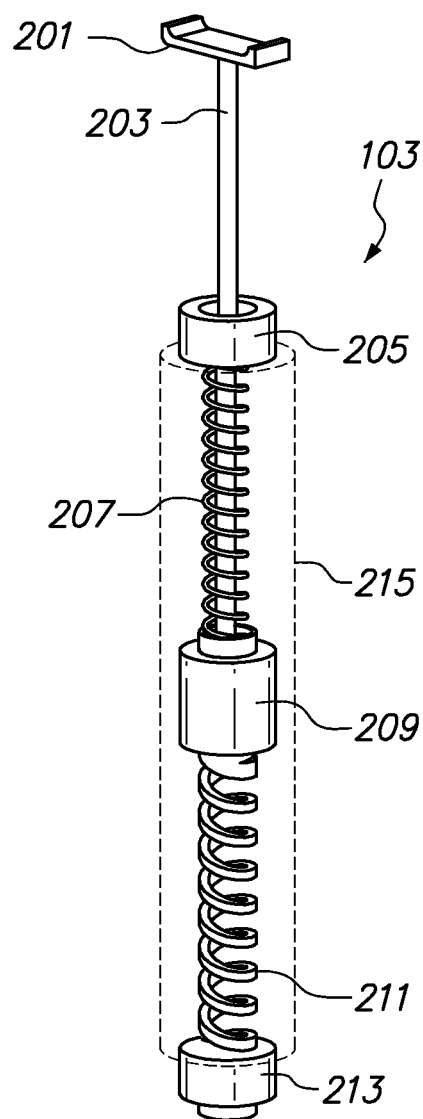
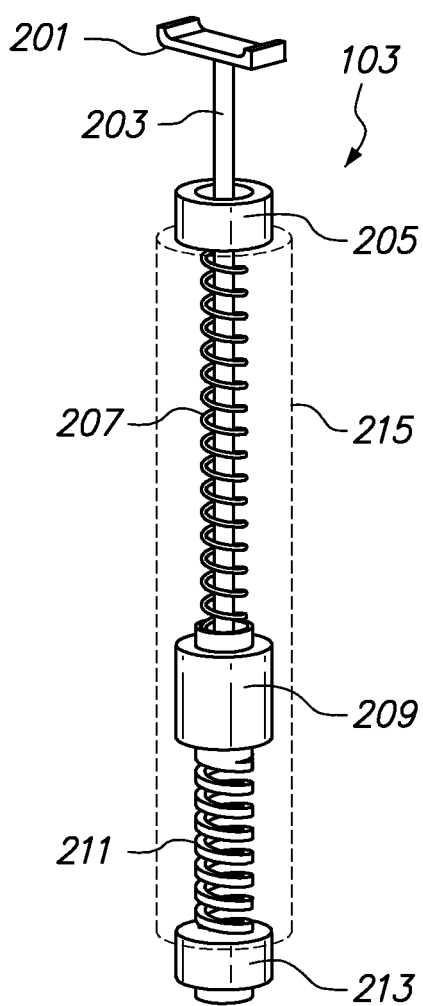


FIG. 2B

FIG. 2C

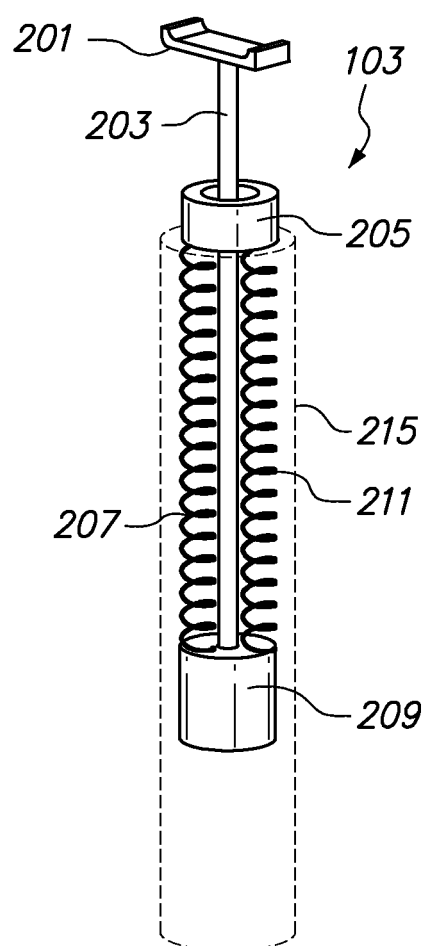
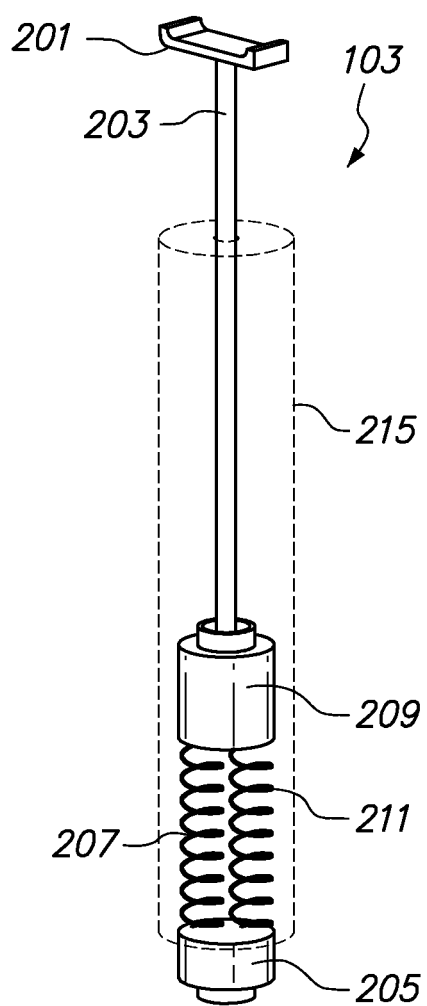
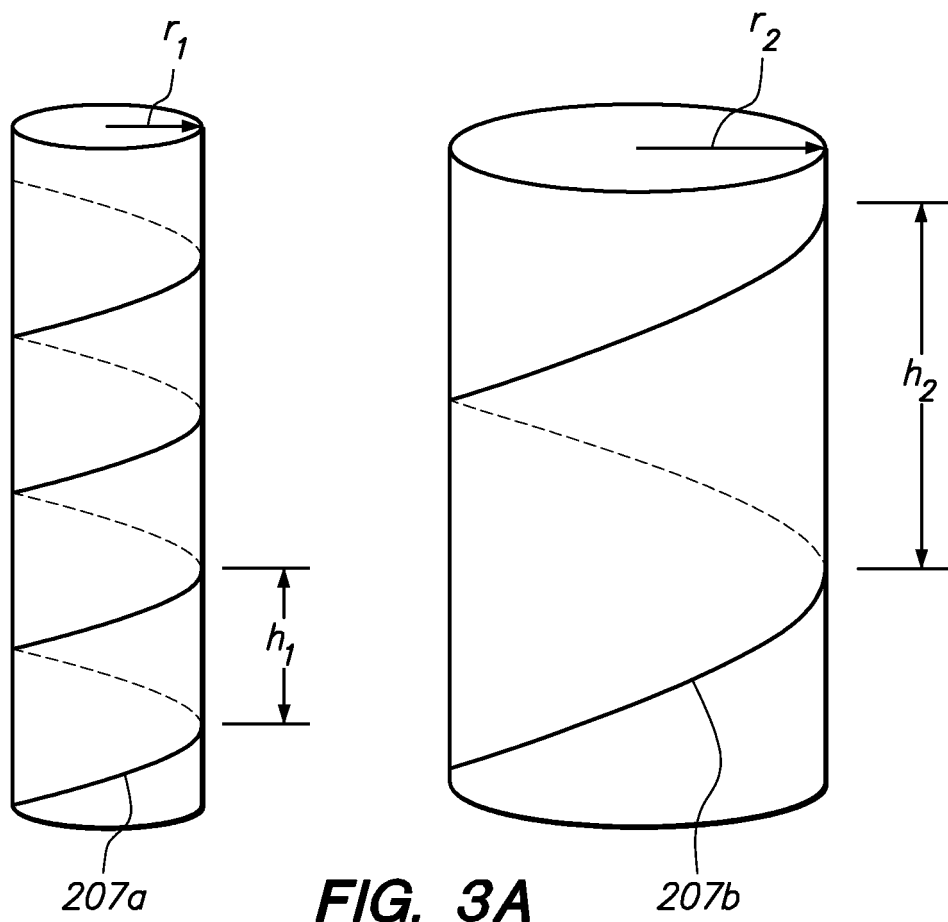


FIG. 2D



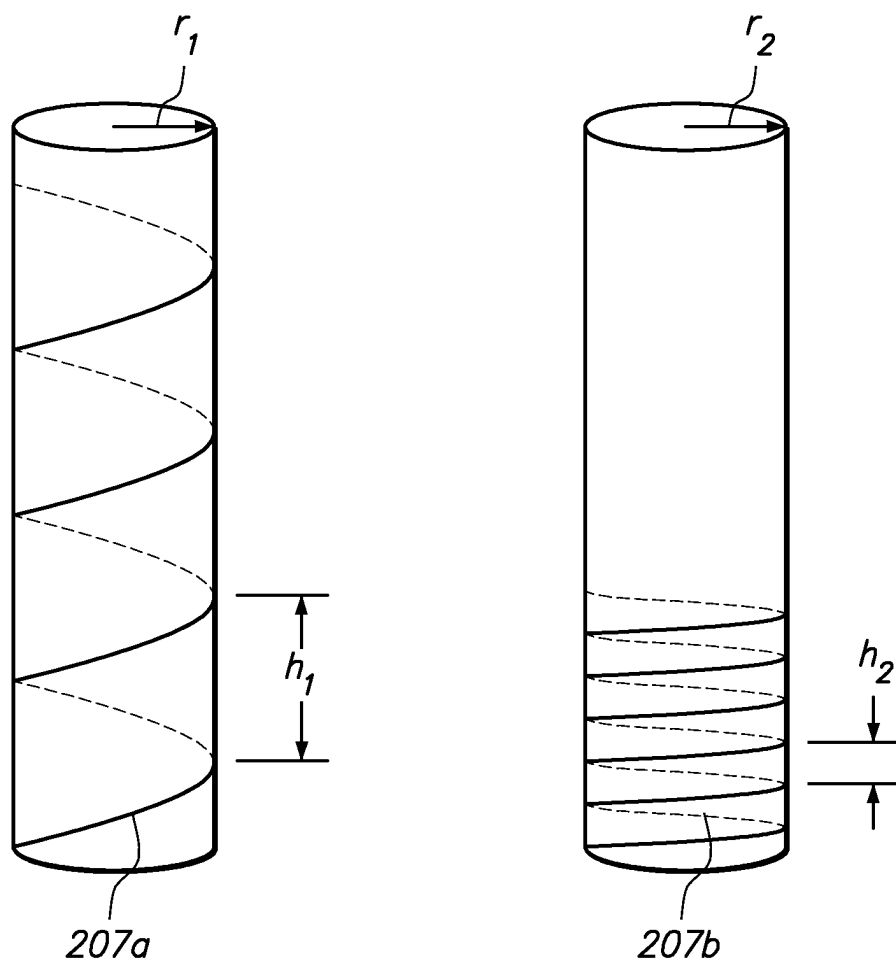


FIG. 3B

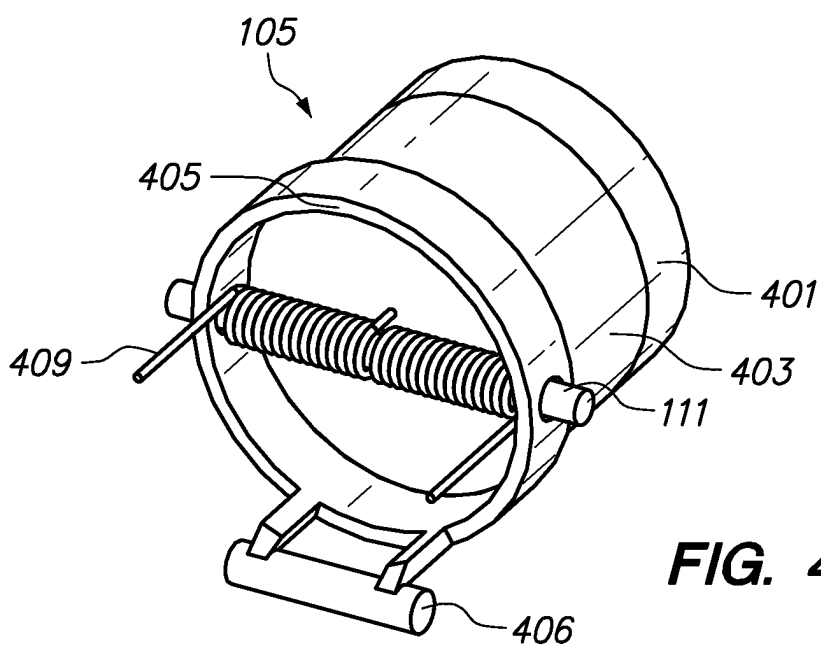


FIG. 4A

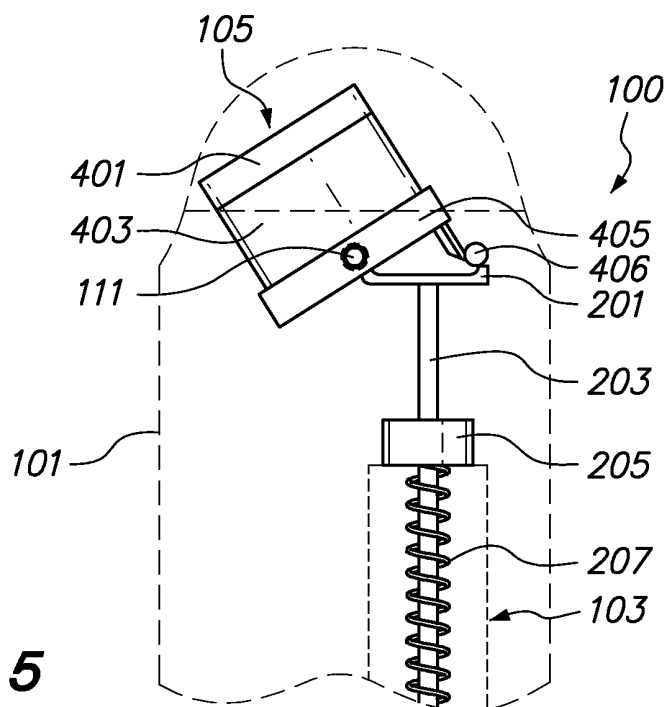
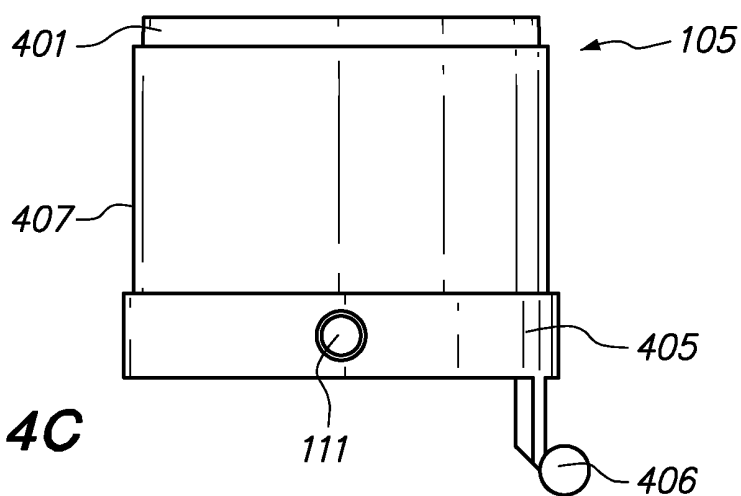
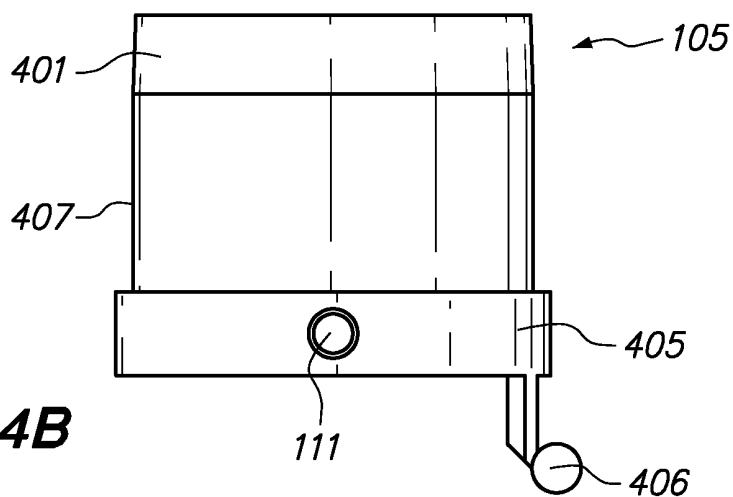


FIG. 6A

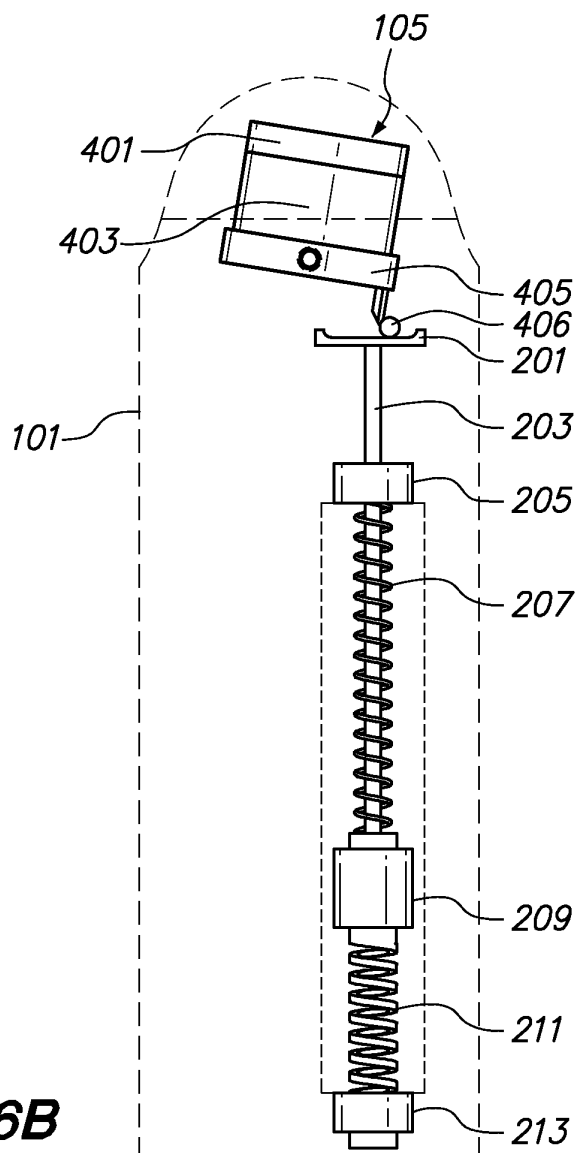
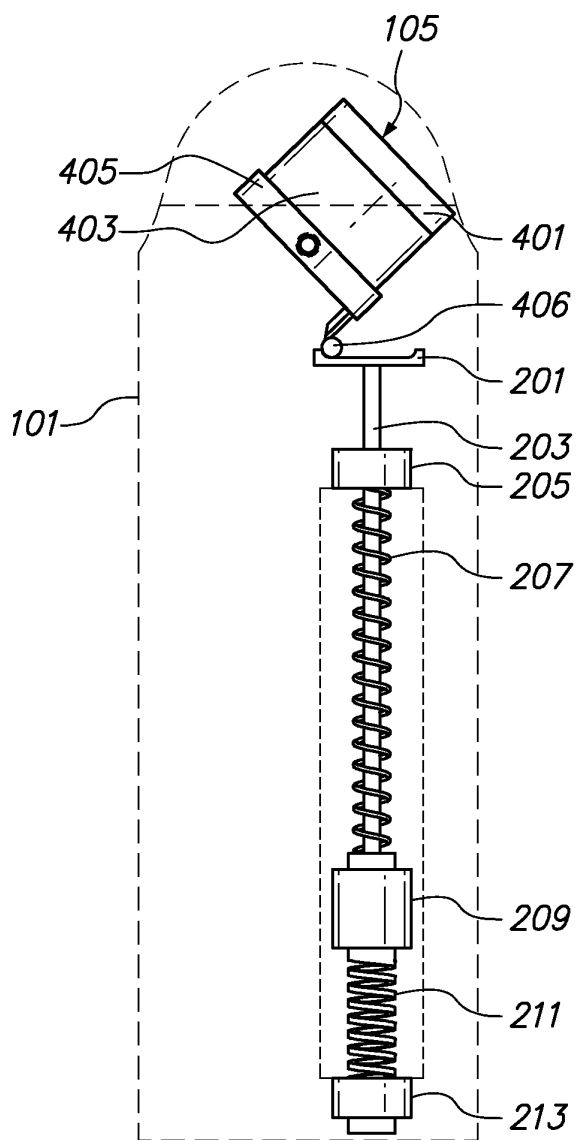


FIG. 6B

FIG. 6C

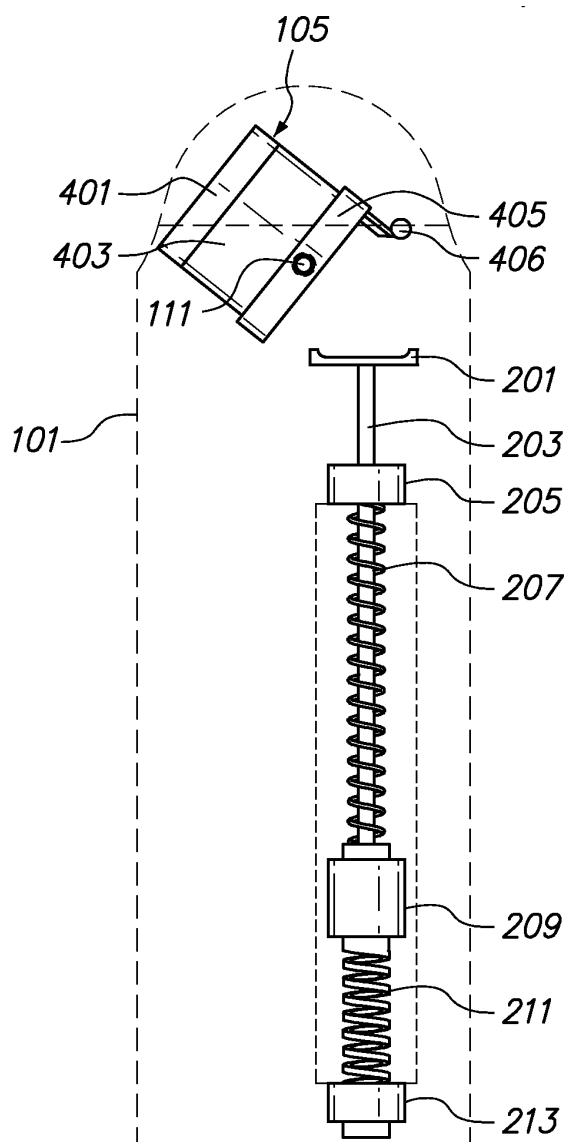
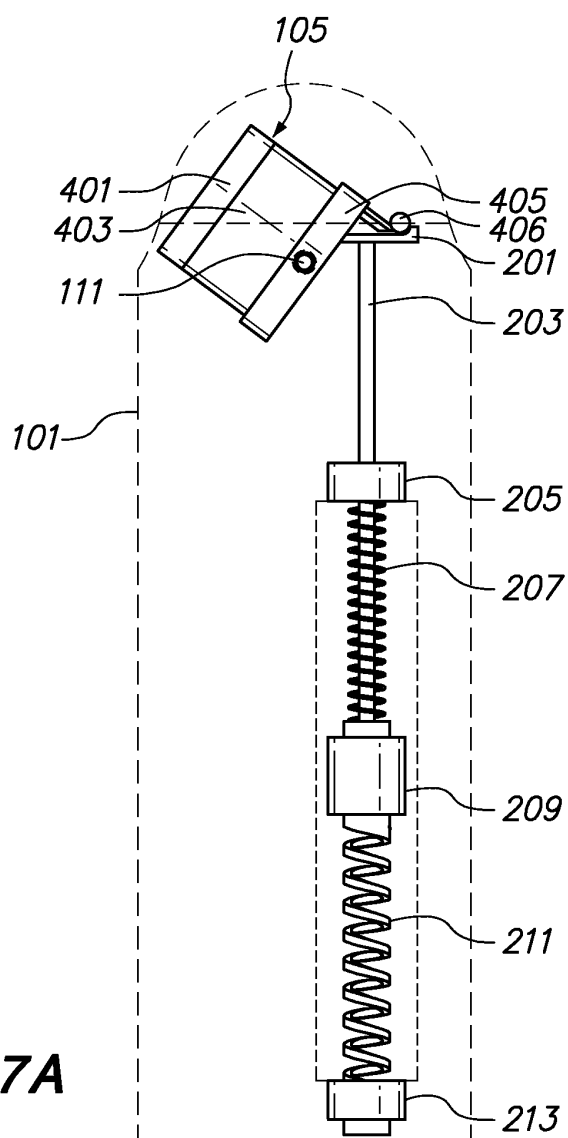


FIG. 7A



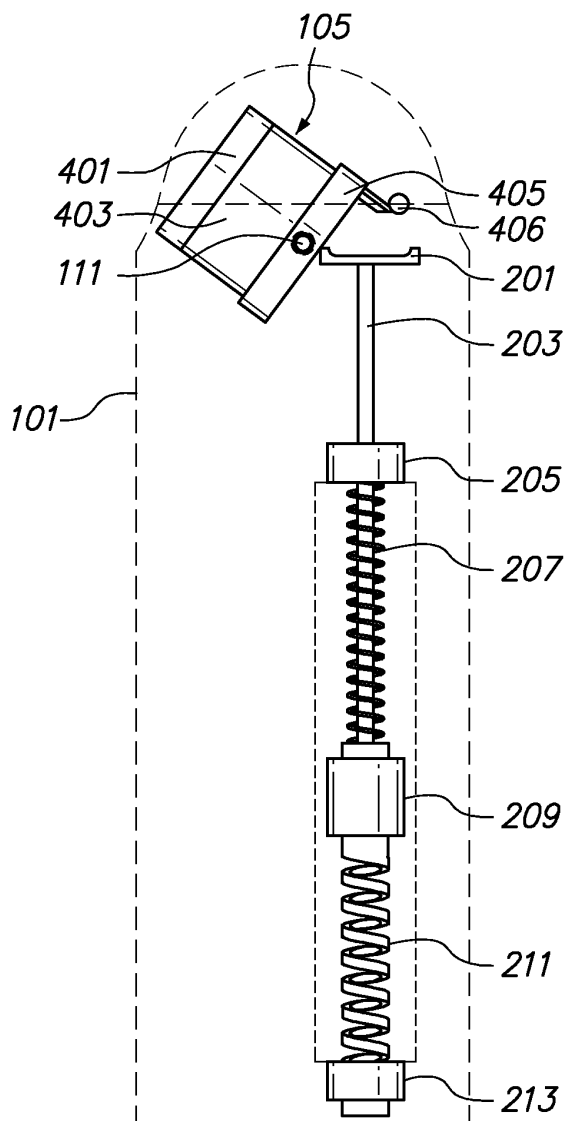


FIG. 7B

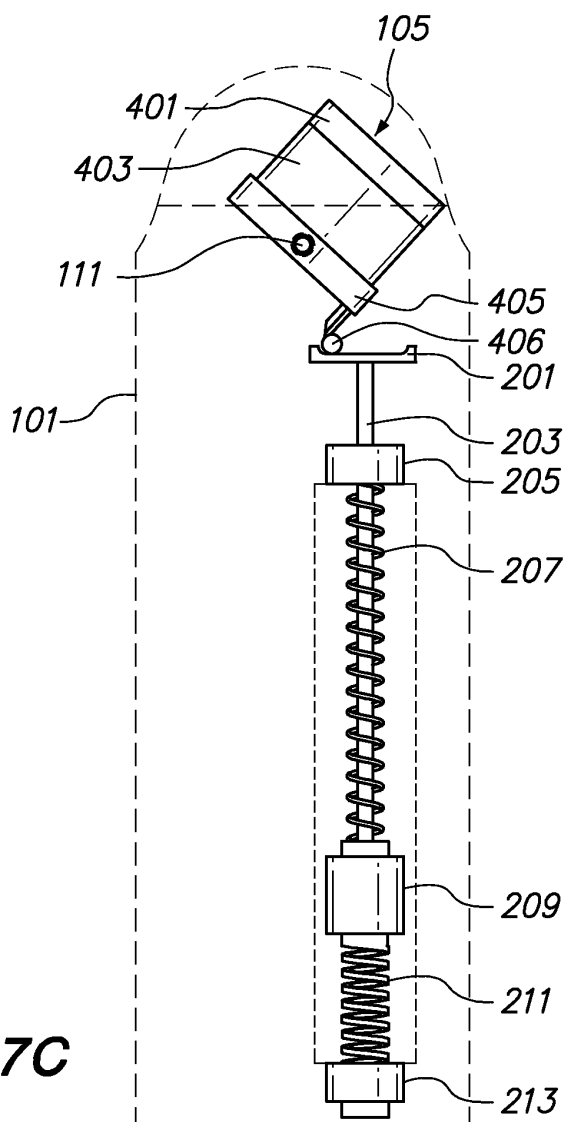


FIG. 7C

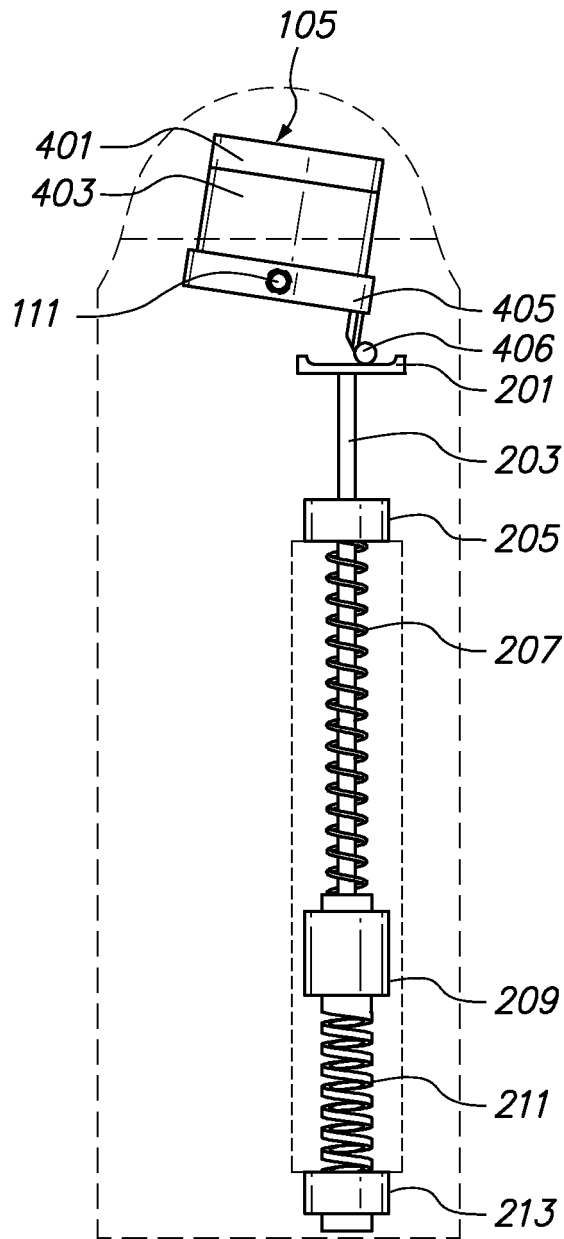


FIG. 7D

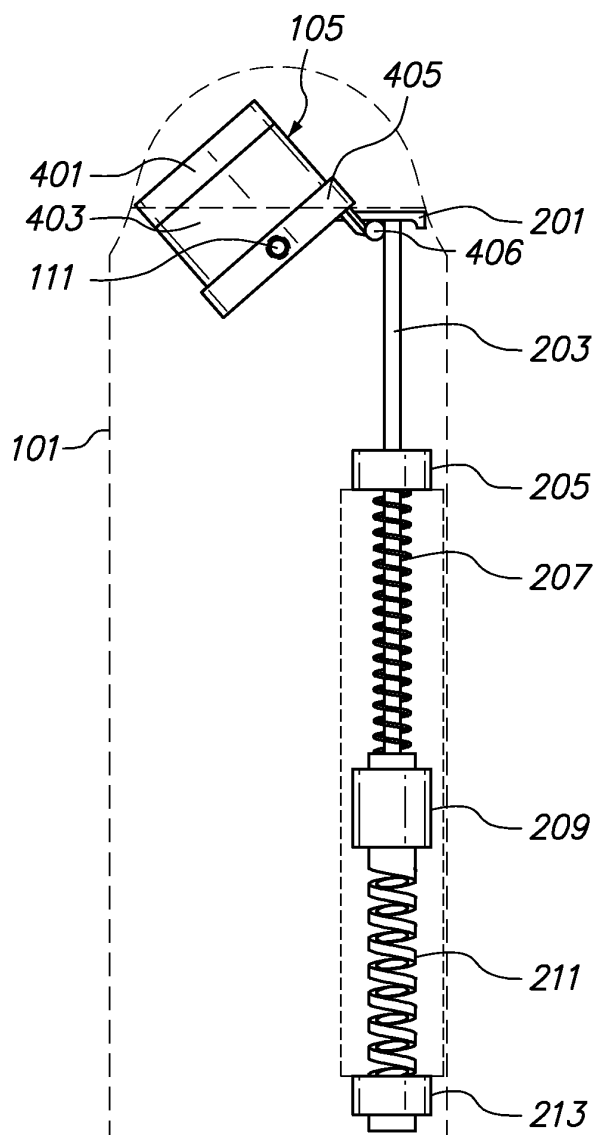


FIG. 8A

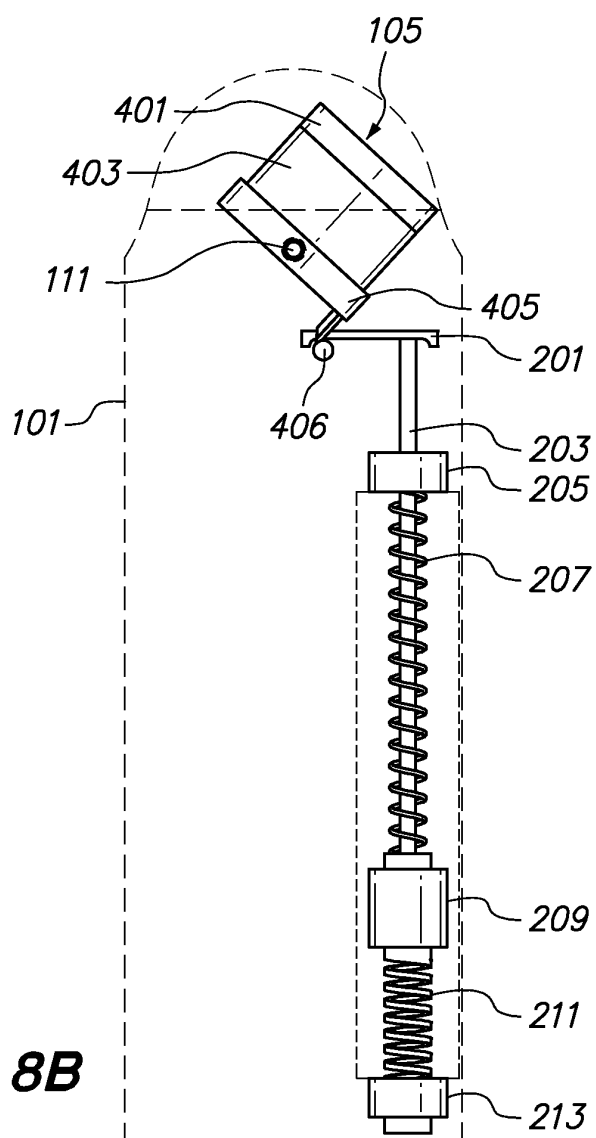


FIG. 8B

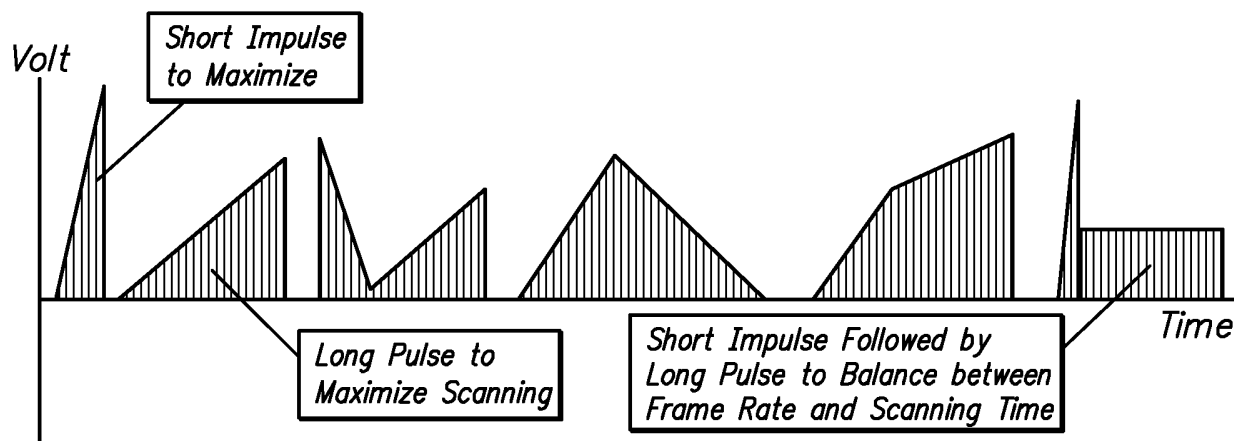


FIG. 9A

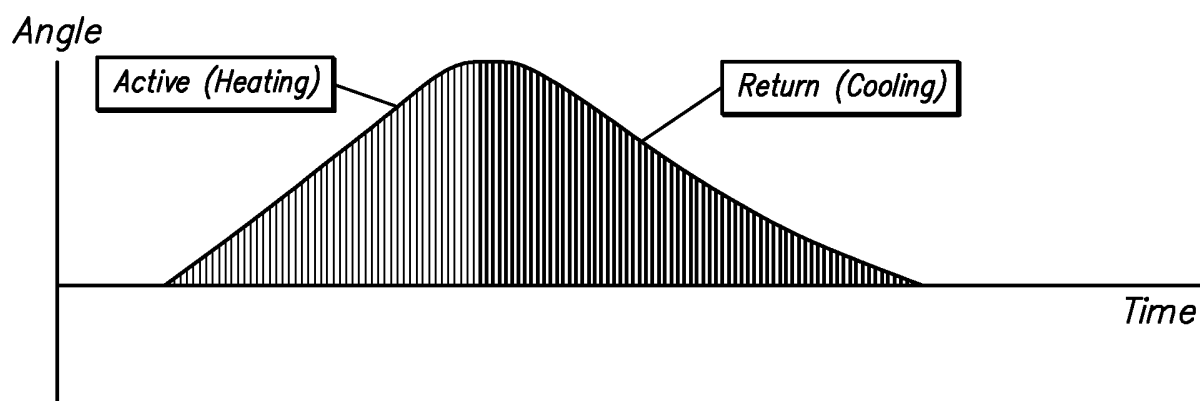


FIG. 9B

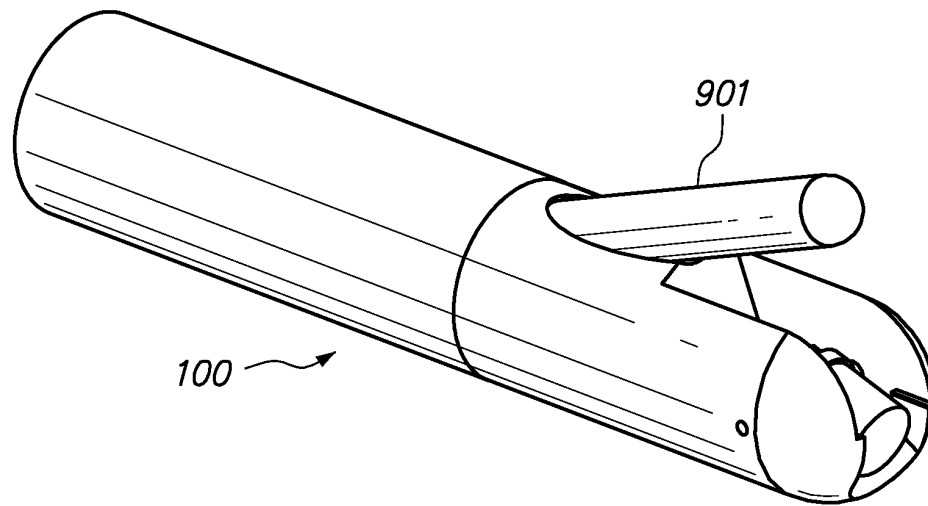


FIG. 10A

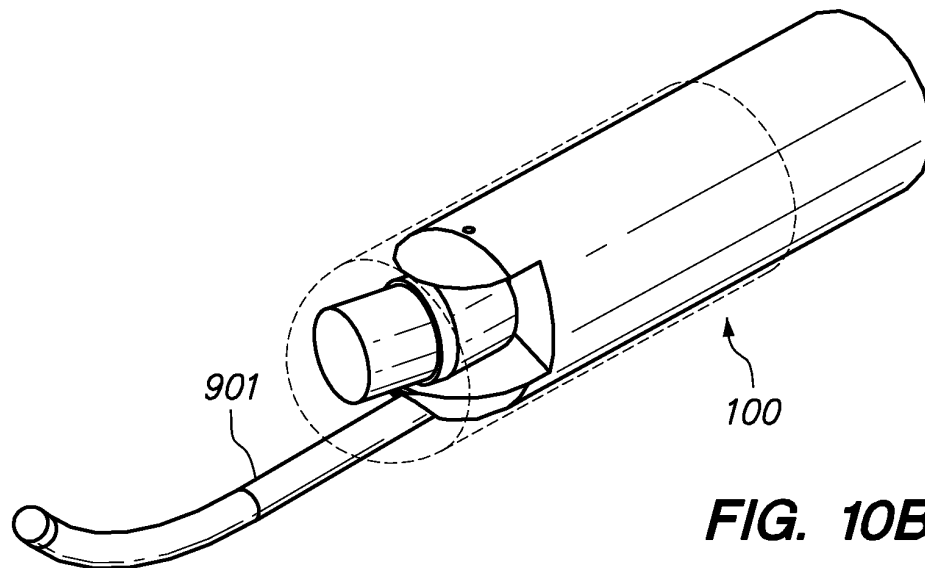


FIG. 10B

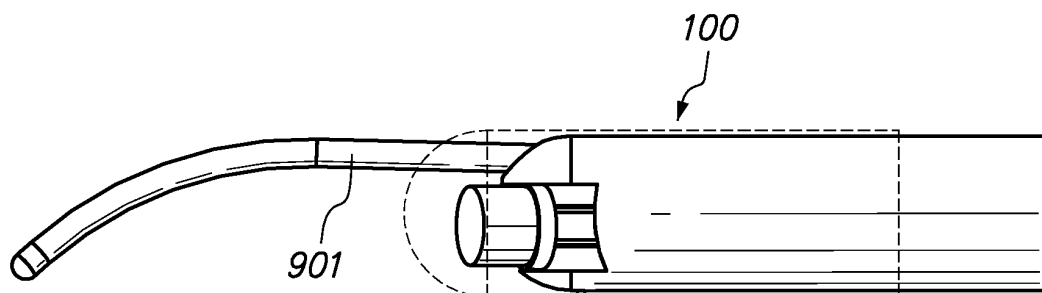


FIG. 10C

REFERENCES CITED IN THE DESCRIPTION

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Patent documents cited in the description

- US 5379772 A [0005]

专利名称(译)	通过局部形状记忆合金致动器实现的微型前视超声成像机制		
公开(公告)号	EP2296553A4	公开(公告)日	2017-03-08
申请号	EP2009747722	申请日	2009-05-15
[标]申请(专利权)人(译)	流体医疗		
[标]发明人	PARK BYONG HO LEVY OREN		
发明人	PARK, BYONG-HO LEVY, OREN		
IPC分类号	A61B8/12 A61B1/01 A61B5/027 A61B5/00 A61B8/00 G01S15/89		
CPC分类号	A61B8/12 A61B8/445 A61B8/4466 A61B8/4494 A61B5/0066 A61B5/0084 G01S7/52079 G01S15/894 Y10T29/49005 A61B5/445 A61B8/4444 A61B8/4461		
代理机构(译)	严实, CORNELIS MARINUS		
优先权	61/054063 2008-05-16 US 61/077111 2008-06-30 US		
其他公开文献	EP2296553A2 EP2296553B1		
外部链接	Espacenet		

摘要(译)

本发明涉及一种新的前视超声装置，其包括嵌入细长构件（例如导丝或导管）内的局部致动器。本发明包括超声换能器元件，其配置成至少在超声换能器元件和局部致动器接合时与局部致动器接合并围绕旋转轴旋转。还公开了使用它们的方法。