



(11) **EP 1 860 994 B1**

(12) **EUROPEAN PATENT SPECIFICATION**

(45) Date of publication and mention  
of the grant of the patent:  
**16.10.2019 Bulletin 2019/42**

(21) Application number: **06736798.7**

(22) Date of filing: **01.03.2006**

(51) Int Cl.:  
**A61B 5/00 (2006.01)**

(86) International application number:  
**PCT/US2006/007537**

(87) International publication number:  
**WO 2006/094169 (08.09.2006 Gazette 2006/36)**

(54) **MULTIPLE WAVELENGTH SENSOR EMITTERS**

EMITTER FÜR EINEN MULTI-WELLENLÄNGEN-SENSOR

EMETTEURS DE CAPTEUR A LONGUEURS D'ONDE MULTIPLES

(84) Designated Contracting States:  
**AT BE BG CH CY CZ DE DK EE ES FI FR GB GR  
HU IE IS IT LI LT LU LV MC NL PL PT RO SE SI  
SK TR**

(30) Priority: **01.03.2005 US 657596 P  
01.03.2005 US 657759 P  
01.03.2005 US 657268 P  
01.03.2005 US 657281 P**

(43) Date of publication of application:  
**05.12.2007 Bulletin 2007/49**

(73) Proprietor: **Masimo Laboratories, Inc.  
Irvine, CA 92618 (US)**

(72) Inventors:  
• **AL-ALI, Ammar  
Tustin, CA 92782 (US)**

- **DIAB, Mohamed  
Mission Viejo, CA 92692 (US)**
- **LAMEGO, Marcelo  
Rancho Santa Margarita, CA 92688 (US)**
- **SMITH, Robert  
Lake Forest, CA 92630 (US)**
- **DALKE, David  
Irvine, CA 92614 (US)**

(74) Representative: **Vossius & Partner  
Patentanwälte Rechtsanwälte mbB  
Siebertstrasse 3  
81675 München (DE)**

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## Description

### BACKGROUND OF THE INVENTION

**[0001]** Spectroscopy is a common technique for measuring the concentration of organic and some inorganic constituents of a solution. The theoretical basis of this technique is the Beer-Lambert law, which states that the concentration  $c_i$  of an absorbent in solution can be determined by the intensity of light transmitted through the solution, knowing the pathlength  $d_\lambda$ , the intensity of the incident light  $I_{0,\lambda}$ , and the extinction coefficient  $\varepsilon_{i,\lambda}$  at a particular wavelength  $\lambda$ . In generalized form, the Beer-Lambert law is expressed as:

$$I_\lambda = I_{0,\lambda} e^{-d_\lambda \cdot \mu_{a,\lambda}} \quad (1)$$

$$\mu_{a,\lambda} = \sum_{i=1}^n \varepsilon_{i,\lambda} \cdot c_i$$

(2)

where  $\mu_{a,\lambda}$  is the bulk absorption coefficient and represents the probability of absorption per unit length. The minimum number of discrete wavelengths that are required to solve EQS. 1-2 are the number of significant absorbers that are present in the solution.

**[0002]** A practical application of this technique is pulse oximetry, which utilizes a noninvasive sensor to measure oxygen saturation (SpO<sub>2</sub>) and pulse rate. In general, the sensor has light emitting diodes (LEDs) that transmit optical radiation of red and infrared wavelengths into a tissue site and a detector that responds to the intensity of the optical radiation after absorption (e.g., by transmission or transreflectance) by pulsatile arterial blood flowing within the tissue site. Based on this response, a processor determines measurements for SpO<sub>2</sub>, pulse rate, and can output representative plethysmographic waveforms. Thus, "pulse oximetry" as used herein encompasses its broad ordinary meaning known to one of skill in the art, which includes at least those noninvasive procedures for measuring parameters of circulating blood through spectroscopy. Moreover, "plethysmograph" as used herein (commonly referred to as "photoplethysmograph"), encompasses its broad ordinary meaning known to one of skill in the art, which includes at least data representative of a change in the absorption of particular wavelengths of light as a function of the changes in body tissue resulting from pulsing blood. Pulse oximeters capable of reading through motion induced noise are available from Masimo Corporation ("Masimo") of Irvine, California. Moreover, portable and other oximeters capable of reading through motion induced noise are disclosed

in at least U.S. Pat. Nos. 6,770,028, 6,658,276, 6,157,850, 6,002,952 5,769,785, and 5,758,644, which are owned by Masimo. Such reading through motion oximeters have gained rapid acceptance in a wide variety of medical applications, including surgical wards, intensive care and neonatal units, general wards, home care, physical training, and virtually all types of monitoring scenarios.

**[0003]** US 2002/0021269 A1 discloses a system and/or method for controlling a display array without the use of row and column drivers. The display elements within the system are configured to maintain an active address signal in response to a received signal containing serially encoded display settings.

**[0004]** US 2004/0081621 A1 relates to an imaging method, wherein an object to be examined is treated with an optically activatable contrast medium and illuminated via a plurality of LEDs.

**[0005]** US 6,253,097 B1 discloses a medical monitoring instrument such as a pulse oximeter which uses vertical cavity surface emitting laser diodes (VCSELs) to produce at least two high intensity, essentially monochromatic light beams.

### SUMMARY OF THE INVENTION

**[0006]** The present invention is defined by the features of the independent claims. Further preferred embodiments are defined in the dependent claims.

In particular, there is a need to noninvasively measure multiple physiological parameters, other than, or in addition to, oxygen saturation and pulse rate. For example, hemoglobin species that are also significant under certain circumstances are carboxyhemoglobin and methemoglobin. Other blood parameters that may be measured to provide important clinical information are fractional oxygen saturation, total hemoglobin (Hbt), bilirubin and blood glucose, to name a few.

The following aspects are useful for the understanding of the present invention but do not fall under the presently claimed invention.

**[0007]** One aspect of a physiological sensor is light emitting sources, each activated by addressing at least one row and at least one column of an electrical grid. The light emitting sources transmit light having multiple wavelengths and a detector is responsive to the transmitted light after attenuation by body tissue.

**[0008]** Another aspect of a physiological sensor is light emitting sources capable of transmitting light having multiple wavelengths. Each of the light emitting sources includes a first contact and a second contact. The first contacts of a first set of the light emitting sources are in communication with a first conductor and the second contacts of a second set of the light emitting sources are in communication with a second conductor. A detector is capable of detecting the transmitted light attenuated by body tissue and outputting a signal indicative of at least one

physiological parameter of the body tissue. At least one light emitting source of the first set and at least one light emitting source of the second set are not common to the first and second sets. Further, each of the first set and the second set comprises at least two of the light emitting sources. US 6,122,042 discloses an apparatus for photometric analysis and/or identification of properties of a material object which comprises a collection of light sources having substantially distinct wavelength envelopes and activated in a rapid sequence of distinct combinations.

**[0009]** A further aspect of a physiological sensor sequentially addresses light emitting sources using conductors of an electrical grid so as to emit light having multiple wavelengths that when attenuated by body tissue is indicative of at least one physiological characteristic. The emitted light is detected after attenuation by body tissue.

#### BRIEF DESCRIPTION OF THE DRAWINGS

##### **[0010]**

FIG. 1 is a perspective view of a physiological measurement system utilizing a multiple wavelength sensor;

FIGS. 2A-C are perspective views of multiple wavelength sensor embodiments in line with the present invention;

FIG. 3 is a general block diagram of a multiple wavelength sensor and sensor controller;

FIG. 4 is an exploded perspective view of a multiple wavelength sensor embodiment in line with the present invention;

FIG. 5 is a general block diagram of an emitter assembly;

FIG. 6 is a perspective view of an emitter assembly embodiment in line with the present invention;

FIG. 7 is a general block diagram of an emitter array;

FIG. 8 is a schematic diagram of an emitter array embodiment in line with the present invention;

FIG. 9 is a general block diagram of equalization;

FIGS. 10A-D are block diagrams of various equalization embodiments;

FIGS. 11A-C are perspective views of an emitter assembly incorporating various equalization embodiments in line with the present invention;

FIG. 12 is a general block diagram of an emitter substrate;

FIGS. 13-14 are top and detailed side views of an emitter substrate embodiment in line with the present invention;

FIG. 15-16 are top and bottom component layout views of an emitter substrate embodiment;

FIG. 17 is a schematic diagram of an emitter substrate embodiment in line with the present invention;

FIG. 18 is a plan view of an inner layer of an emitter substrate embodiment in line with the present inven-

tion;

FIG. 19 is a general block diagram of an interconnect assembly in relationship to other sensor assemblies;

FIG. 20 is a block diagram of an interconnect assembly embodiment in line with the present invention;

FIG. 21 is a partially-exploded perspective view of a flex circuit assembly of an interconnect assembly;

FIG. 22 is a top plan view of a flex circuit;

FIG. 23 is an exploded perspective view of an emitter portion of a flex circuit assembly;

FIG. 24 is an exploded perspective view of a detector assembly.

FIGS. 25-26 are block diagrams of adjacent detector and stacked detector

FIG. 27 is a block diagram of a finger clip embodiment of an attachment assembly;

FIG. 28 is a general block diagram of a detector pad;

FIGS. 29A-B are perspective views of detector pad;

FIGS. 30A-H are perspective bottom, perspective top, bottom, back, top, side cross sectional, side, and front cross sectional views of an emitter pad embodiment;

FIGS. 31A-H are perspective bottom, perspective top, top, back, bottom, side cross sectional, side, and front cross sectional views of a detector pad embodiment;

FIGS. 32A-H are perspective bottom, perspective top, top, back, bottom, side cross sectional, side, and front cross sectional views of a shoe box;

FIGS. 33A-H are perspective bottom, perspective top, top, back, bottom, side cross sectional, side, and front cross sectional views of a slim-finger emitter pad embodiment;

FIGS. 34A-H are perspective bottom, perspective top, top, back, bottom, side cross sectional, side, and front cross sectional views of a slim-finger detector pad embodiment;

FIGS. 35A-B are plan and cross sectional views, respectively, of a spring assembly embodiment;

FIGS. 36A-C are top, perspective and side views of a finger clip spring;

FIGS. 37A-D are top, back, bottom, and side views of a spring plate;

FIGS. 38A-D are front cross sectional, bottom, front and side cross sectional views of an emitter-pad shell;

FIGS. 39A-D are back, top, front and side cross sectional views of a detector-pad shell;

FIG. 40 is a general block diagram of a monitor and a sensor;

FIGS. 41A-C are schematic diagrams of grid drive for a sensor having back-to-back diodes and an information element;

FIGS. 42 is a schematic diagrams of a grid drive embodiment in line with the present invention for an information element;

FIGS. 43A-C are schematic diagrams for grid drive readable information elements;

FIGS. **44A-B** are cross sectional and side cut away views of a sensor cable;  
 FIG. **45** is a block diagram of a sensor controller, and  
 FIG. **46** is a detailed exploded perspective view of a multiple wavelength sensor embodiment in line with the present invention.

## DETAILED DESCRIPTION OF THE PREFERRED EMBODIMENTS

### Overview

[0011] In this application, reference is made to many blood parameters. Some references that have common shorthand designations are referenced through such shorthand designations. For example, as used herein, HbCO designates carboxyhemoglobin, HbMet designates methemoglobin, and Hbt designates total hemoglobin. Other shorthand designations such as COHb, MetHb, and tHb are also common in the art for these same constituents. These constituents are generally reported in terms of a percentage, often referred to as saturation, relative concentration or fractional saturation. Total hemoglobin is generally reported as a concentration in g/dL. The use of the particular shorthand designators presented in this application does not restrict the term to any particular manner in which the designated constituent is reported.

[0012] FIG. 1 illustrates a physiological measurement system **10** having a monitor **100** and a multiple wavelength sensor assembly **200** with enhanced measurement capabilities as compared with conventional pulse oximetry. The physiological measurement system **10** allows the monitoring of a person, including a patient. In particular, the multiple wavelength sensor assembly **200** allows the measurement of blood constituent and related parameters. In addition to oxygen saturation and pulse rate. Alternatively, the multiple wavelength sensor assembly **200** allows the measurement of oxygen saturation and pulse rate with increased accuracy or robustness as compared with conventional pulse oximetry.

[0013] The sensor assembly **200** is configured to plug into a monitor sensor port **110**. Monitor keys **160** provide control over operating modes and alarms, to name a few. A display **170** provides readouts of measured parameters, such as oxygen saturation, pulse rate, HbCO and HbMet to name a few.

[0014] FIGS. **2A** illustrates a multiple wavelength sensor assembly **200** having a sensor **400** adapted to attach to a tissue site, a sensor cable **4400** and a monitor connector **210**. The sensor **400** is incorporated into a reusable finger clip adapted to removably attach to, and transmit light through, a fingertip. The sensor cable **4400** and monitor connector **210** are integral to the sensor **400**, as shown. Alternatively, the sensor **400** may be configured separately from the cable **4400** and connector **210**.

[0015] FIGS. **2B-C** illustrate alternative sensors, including a sensor **401** (FIG. **2B**) partially disposable and

partially reusable (resposable) and utilizing an adhesive attachment mechanism. Also shown is a sensor **402** (FIG. **2C**) being disposable and utilizing an adhesive attachment mechanism.

5 [0016] A sensor may be configured to attach to various tissue sites other than a finger, such as a foot or an ear. Also a sensor may be configured as a reflectance or transreflectance device that attaches to a forehead or other tissue surface.

10 [0017] FIG. 3 illustrates a sensor assembly **400** having an emitter assembly **500**, a detector assembly **2400**, an interconnect assembly **1900** and an attachment assembly **2700**. The emitter assembly **500** responds to drive signals received from a sensor controller **4500** in the monitor **100** via the cable **4400** so as to transmit optical radiation having a plurality of wavelengths into a tissue site. The detector assembly **2400** provides a sensor signal to the monitor **100** via the cable **4400** in response to optical radiation received after attenuation by the tissue site. The interconnect assembly **1900** provides electrical communication between the cable **4400** and both the emitter assembly **500** and the detector assembly **2400**. The attachment assembly **2700** attaches the emitter assembly **500** and detector assembly **2400** to a tissue site, as described above. The emitter assembly **500** is described in further detail with respect to FIG. 5, below. The interconnect assembly **1900** is described in further detail with respect to FIG. 19, below. The detector assembly **2400** is described in further detail with respect to FIG. 24, below. The attachment assembly **2700** is described in further detail with respect to FIG. 27, below.

35 [0018] FIG. 4 illustrates a sensor **400** that removably attaches to a fingertip. The sensor **400** houses a multiple wavelength emitter assembly **500** and corresponding detector assembly **2400**. A flex circuit assembly **1900** mounts the emitter and detector assemblies **500**, **2400** and interconnects them to a multiwire sensor cable **4400**. Advantageously, the sensor **400** is configured in several respects for both wearer comfort and parameter measurement performance. The flex circuit assembly **1900** is configured to mechanically decouple the cable **4400** wires from the emitter and detector assemblies **500**, **2400** to reduce pad stiffness and wearer discomfort. The pads **3000**, **3100** are mechanically decoupled from shells **3800**, **3900** to increase flexibility and wearer comfort. A spring **3600** is configured in hinged shells **3800**, **3900** so that the pivot point of the finger clip is well behind the fingertip, improving finger attachment and more evenly distributing the clip pressure along the finger.

50 [0019] As shown in FIG. 4, the detector pad **3100** is structured to properly position a fingertip in relationship to the detector assembly **2400**. The pads have flaps that block ambient light. The detector assembly **2400** is housed in an enclosure so as to reduce light piping from the emitter assembly to the detector assembly without passing through fingertip tissue. These and other features are described in detail below. Specifically, emitter assembly embodiments in line with the present invention

are described with respect to FIGS. 5-18. Interconnect assemblies, including the flexible circuit assembly 1900, are described with respect to FIGS. 19-23. Detector assemblies are described with respect to FIGS. 24-26. Attachment assemblies are described with respect to FIGS. 27-39.

#### Emitter Assembly

[0020] FIG. 5 illustrates an emitter assembly 500 having an emitter array 700, a substrate 1200 and equalization 900. The emitter array 700 has multiple light emitting sources, each activated by addressing at least one row and at least one column of an electrical grid. The light emitting sources are capable of transmitting optical radiation having multiple wavelengths. The equalization 900 accounts for differences in tissue attenuation of the optical radiation across the multiple wavelengths so as to at least reduce wavelength-dependent variations in detected intensity. The substrate 1200 provides a physical mount for the emitter array and emitter-related equalization and a connection between the emitter array and the interconnection assembly. Advantageously, the substrate 1200 also provides a bulk temperature measurement so as to calculate the operating wavelengths for the light emitting sources. The emitter array 700 is described in further detail with respect to FIG. 7, below. Equalization is described in further detail with respect to FIG. 9, below. The substrate 1200 is described in further detail with respect to FIG. 12, below.

[0021] FIG. 6 illustrates an emitter assembly 500 embodiment in line with the present invention having an emitter array 700, an encapsulant 600, an optical filter 1100 and a substrate 1200. Various aspects of the emitter assembly 500 are described with respect to FIGS. 7-18, below. The emitter array 700 emits optical radiation having multiple wavelengths of predetermined nominal values, advantageously allowing multiple parameter measurements. In particular, the emitter array 700 has multiple light emitting diodes (LEDs) 710 that are physically arranged and electrically connected in an electrical grid to facilitate drive control, equalization, and minimization of optical pathlength differences at particular wavelengths. The optical filter 1100 is advantageously configured to provide intensity equalization across a specific LED subset. The substrate 1200 is configured to provide a bulk temperature of the emitter array 700 so as to better determine LED operating wavelengths.

#### Emitter Array

[0022] FIG. 7 illustrates an emitter array 700 having multiple light emitters (LE) 710 capable of emitting light 702 having multiple wavelengths into a tissue site 1. Row drivers 4530 and column drivers 4560 are electrically connected to the light emitters 710 and activate one or more light emitters 710 by addressing at least one row 720 and at least one column 740 of an electrical grid. In

one embodiment in line with the present invention, the light emitters 710 each include a first contact 712 and a second contact 714. The first contact 712 of a first subset 730 of light emitters is in communication with a first conductor 720 of the electrical grid. The second contact 714 of a second subset 750 of light emitters is in communication with a second conductor 740. Each subset comprises at least two light emitters, and at least one of the light emitters of the first and second subsets 730, 750 are not in common. A detector 2400 is capable of detecting the emitted light 702 and outputting a sensor signal 2500 responsive to the emitted light 702 after attenuation by the tissue site 1. As such, the sensor signal 2500 is indicative of at least one physiological parameter corresponding to the tissue site 1, as described above.

[0023] FIG. 8 illustrates an emitter array 700 having LEDs 801 connected within an electrical grid of n rows and m columns totaling n + m drive lines 4501, 4502, where n and m integers greater than one. The electrical grid advantageously minimizes the number of drive lines required to activate the LEDs 801 while preserving flexibility to selectively activate individual LEDs 801 in any sequence and multiple LEDs 801 simultaneously. The electrical grid also facilitates setting LED currents so as to control intensity at each wavelength, determining operating wavelengths and monitoring total grid current so as to limit power dissipation. The emitter array 700 is also physically configured in rows 810. This physical organization facilitates clustering LEDs 801 according to wavelength so as to minimize pathlength variations and facilitates equalization of LED intensities.

[0024] As shown in FIG. 8, one embodiment in line with the present invention of an emitter array 700 comprises up to sixteen LEDs 801 configured in an electrical grid of four rows 810 and four columns 820. Each of the four row drive lines 4501 provide a common anode connection to four LEDs 801, and each of the four column drive lines 4502 provide a common cathode connection to four LEDs 801. Thus, the sixteen LEDs 801 are advantageously driven with only eight wires, including four anode drive lines 812 and four cathode drive lines 822. This compares favorably to conventional common anode or cathode LED configurations, which require more drive lines. In a particular embodiment in line with the present invention, the emitter array 700 is partially populated with eight LEDs having nominal wavelengths as shown in TABLE 1. Further, LEDs having wavelengths in the range of 610-630 nm are grouped together in the same row. The emitter array 700 is adapted to a physiological measurement system 10 (FIG. 1) for measuring H<sub>b</sub>CO and/or METHb in addition to S<sub>p</sub>O<sub>2</sub> and pulse rate.

TABLE 1: Nominal LED Wavelengths

LED	$\lambda$	Row	Col
D1	630	1	1
D2	620	1	2

(continued)

LED	$\lambda$	Row	Col
D3	610	1	3
D4		1	4
D5	700	2	1
D6	730	2	2
D7	660	2	3
D8	805	2	4
D9		3	1
D10		3	2
D11		3	3
D12	905	3	4
D13		4	1
D14		4	2
D15		4	3
D16		4	4

**[0025]** Also shown in FIG. 8, row drivers **4530** and column drivers **4560** located in the monitor **100** selectively activate the LEDs **801**. In particular, row and column drivers **4530**, **4560** function together as switches to Vcc and current sinks, respectively, to activate LEDs and as switches to ground and Vcc, respectively, to deactivate LEDs. This push-pull drive configuration advantageously prevents parasitic current flow in deactivated LEDs. In a particular embodiment in line with the present invention, only one row drive line **4501** is switched to Vcc at a time. One to four column drive lines **4502**, however, can be simultaneously switched to a current sink so as to simultaneously activate multiple LEDs within a particular row. Activation of two or more LEDs of the same wavelength facilitates intensity equalization, as described with respect to FIGS. 9-11, below. LED drivers are described in further detail with respect to FIG. 45, below.

**[0026]** Although an emitter assembly is described above with respect to an array of light emitters each configured to transmit optical radiation centered around a nominal wavelength, in another embodiment, an emitter assembly advantageously utilizes one or more tunable broadband light sources, including the use of filters to select the wavelength, so as to minimize wavelength-dependent pathlength differences from emitter to detector. In yet another emitter assembly embodiment, optical radiation from multiple emitters each configured to transmit optical radiation centered around a nominal wavelength is funneled to a tissue site point so as to minimize wavelength-dependent pathlength differences. This funneling may be accomplished with fiber optics or mirrors, for example. In further embodiments, the LEDs **801** can be configured with alternative orientations with correspond-

ingly different drivers among various other configurations of LEDs, drivers and interconnecting conductors.

#### Equalization

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**[0027]** FIG. 9 illustrate a physiological parameter measurement system **10** having a controller **4500**, an emitter assembly **500**, a detector assembly **2400** and a front-end **4030**. The emitter assembly **500** is configured to transmit optical radiation having multiple wavelengths into the tissue site **1**. The detector assembly **2400** is configured to generate a sensor signal **2500** responsive to the optical radiation after tissue attenuation. The front-end **4030** conditions the sensor signal **2500** prior to analog-to-digital conversion (ADC).

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**[0028]** FIG. 9 also generally illustrates equalization **900** in a physiological measurement system **10** operating on a tissue site **1**. Equalization encompasses features incorporated into the system **10** in order to provide a sensor signal **2500** that falls well within the dynamic range of the ADC across the entire spectrum of emitter wavelengths. In particular, equalization compensates for the imbalance in tissue light absorption due to Hb and HbO<sub>2</sub> **910**. Specifically, these blood constituents attenuate red wavelengths greater than IR wavelengths. Ideally, equalization **900** balances this unequal attenuation. Equalization **900** can be introduced anywhere in the system **10** from the controller **4500** to front-end **4000** and can include compensatory attenuation versus wavelength, as shown, or compensatory amplification versus or both.

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**[0029]** Equalization can be achieved to a limited extent by adjusting drive currents from the controller **4500** and front-end **4030** amplification accordingly to wavelength so as to compensate for tissue absorption characteristics. Signal demodulation constraints, however, limit the magnitude of these adjustments. Advantageously, equalization **900** is also provided along the optical path from emitters **500** to detector **2400**. Equalization embodiments in line with the present invention are described in further detail with respect to FIGS. 10-11, below.

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**[0030]** FIGS. 10A-D illustrate various equalization embodiments having an emitter array **700** adapted to transmit optical radiation into a tissue site **1** and a detector assembly **2400** adapted to generate a sensor signal **2500** responsive to the optical radiation after tissue attenuation. FIG. 10A illustrates an optical filter **1100** that attenuates at least a portion of the optical radiation before it is transmitted into a tissue site **1**. In particular, the optical filter **1100** attenuates at least a portion of the IR wavelength spectrum of the optical radiation so as to approximate an equalization curve **900** (FIG. 9). FIG. 10B illustrates an optical filter **1100** that attenuates at least a portion of the optical radiation after it is attenuated by a tissue site **1**, where the optical filter **1100** approximates an equalization curve **900** (FIG. 9).

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**[0031]** FIG. 10C illustrates an emitter array **700** where at least a portion of the emitter array generates one or more wavelengths from multiple light emitters **710** of the

same wavelength. In particular, the same-wavelength light emitters **710** boost at least a portion of the red wavelength spectrum so as to approximately equalize the attenuation curves **910** (FIG. 9). FIG. **10D** illustrates a detector assembly **2400** having multiple detectors **2610**, **2620** selected so as to equalize the attenuation curves **910** (FIG. 9). To a limited extent, optical equalization can also be achieved by selection of particular emitter array **700** and detector **2400** components, e.g. LEDs having higher output intensities or detectors having higher sensitivities at red wavelengths. Although equalization embodiments are described above with respect to red and IR wavelengths, these equalization embodiments can be applied to equalize tissue characteristics across any portion of the optical spectrum.

**[0032]** FIGS. **11A-C** illustrates an optical filter **1100** for an emitter assembly **500** that advantageously provides optical equalization, as described above. LEDs within the emitter array **700** may be grouped according to output intensity or wavelength or both. Such a grouping facilitates equalization of LED intensity across the array. In particular, relatively low tissue absorption and/or relatively high output intensity LEDs can be grouped together under a relatively high attenuation optical filter. Likewise, relatively low tissue absorption and/or relatively low output intensity LEDs can be grouped together without an optical filter or under a relatively low or negligible attenuation optical filter. Further, high tissue absorption and/or low intensity LEDs can be grouped within the same row with one or more LEDs of the same wavelength being simultaneously activated, as described with respect to FIG. **10C**, above. In general, there can be any number of LED groups and any number of LEDs within a group. There can also be any number of optical filters corresponding to the groups having a range of attenuation, including no optical filter and/or a "clear" filter having negligible attenuation.

**[0033]** As shown in FIGS. **11A-C**, a filtering media may be advantageously added to an encapsulant that functions both as a cover to protect LEDs and bonding wires and as an optical filter **1100**. A filtering media **1100** encapsulates a select group of LEDs and a clear media **600** (FIG. **6**) encapsulates the entire array **700** and the filtering media **1000** (FIG. **6**).

**[0034]** According to TABLE 1, above, five LEDs nominally emitting at 660-905 nm are encapsulated with both a filtering media **1100** and an overlying clear media **600** (FIG. **6**), i.e. attenuated. The filtering media **1100** is a 40:1 mixture of a clear encapsulant (EPO-TEK OG147-7) and an opaque encapsulate (EPO-TEK OG147) both available from Epoxy Technology, Inc., Billerica, MA. Three LEDs nominally emitting at 610-630 nm are only encapsulated with the clear media **600** (FIG. **6**), i.e. unattenuated.

**[0035]** Individual LEDs maybe singly or multiply encapsulated according to tissue absorption and/or output intensity.

**[0036]** Filtering media may be separately attachable

optical filters or a combination of encapsulants and separately attachable optical filters.

**[0037]** The emitter assembly **500** may have one or more notches along each side proximate the component end **1305** (FIG. **13**) for retaining one or more clip-on optical filters.

#### Substrate

**[0038]** FIG. **12** illustrates light emitters **710** configured to transmit optical radiation **1201** having multiple wavelengths in response to corresponding drive currents **1210**. A thermal mass **1220** is disposed proximate the emitters **710** so as to stabilize a bulk temperature **1202** for the emitters. A temperature sensor **1230** is thermally coupled to the thermal mass **1220**, wherein the temperature sensor **1230** provides a temperature sensor output **1232** responsive to the bulk temperature **1202** so that the wavelengths are determinable as a function of the drive currents **1210** and the bulk temperature **1202**.

**[0039]** An operating wavelength  $\lambda_a$  of each light emitter **710** may be determined according to EQ. 3

$$\lambda_a = f(T_b, I_{drive}, \sum I_{drive})$$

(3)

where  $T_b$  is the bulk temperature,  $I_{drive}$  is the drive current for a particular light emitter, as determined by the sensor controller **4500** (FIG. **45**), described below, and  $\sum I_{drive}$  is the total drive current for all light emitters.

Temperature sensors are configured to measure the temperature of each light emitter **710** and an operating wavelength  $\lambda_a$  of each light emitter **710** is determined according to EQ. 4

$$\lambda_a = f(T_a, I_{drive}, \sum I_{drive})$$

(4)

where  $T_a$  is the temperature of a particular light emitter,  $I_{drive}$  is the drive current for that light emitter and  $\sum I_{drive}$  is the total drive current for all light emitters.

**[0040]** An operating wavelength for each light emitter is determined by measuring the junction voltage for each light emitter **710**. The temperature of each light emitter **710** is controlled, such as by one or more Peltier cells coupled to each light emitter **710**, and an operating wavelength for each light emitter **710** is determined as a function of the resulting controlled temperature or temperatures.

**[0041]** The operating wavelength for each light emitter **710** can be determined directly, for example by attaching a charge coupled device (CCD) to each light emitter or by attaching a fiberoptic to each light emitter and coupling the fiberoptics to a wavelength measuring device, to

name a few.

[0042] FIGS. 13-18 illustrate a substrate 1200 configured to provide thermal conductivity between an emitter array 700 (FIG. 8) and a thermistor 1540 (FIG. 16). In this manner, the resistance of the thermistor 1540 (FIG. 16) can be measured in order to determine the bulk temperature of LEDs 801 (FIG. 8) mounted on the substrate 1200. The substrate 1200 is also configured with a relatively significant thermal mass, which stabilizes and normalizes the bulk temperature so that the thermistor measurement of bulk temperature is meaningful.

[0043] FIGS. 13-14 illustrate a substrate 1200 having a component side 1301, a solder side 1302, a component end 1305 and a connector end 1306. Alignment notches 1310 are disposed between the ends 1305, 1306. The substrate 1200 further has a component layer 1401, inner layers 1402-1405 and a solder layer 1406. The inner layers 1402-1405, e.g. inner layer 1402 (FIG. 18), have substantial metallized areas 1411 that provide a thermal mass 1220 (FIG. 12) to stabilize a bulk temperature for the emitter array 700 (FIG. 12). The metallized areas 1411 also function to interconnect component pads 1510 and wire bond pads 1520 (FIG. 15) to the connector 1530.

[0044] FIGS. 15-16 illustrate a substrate 1200 having component pads 1510 and wire bond pads 1520 at a component end 1305. The component pads 1510 mount and electrically connect a first side (anode or cathode) of the LEDs 801 (FIG. 8) to the substrate 1200. Wire bond pads 1520 electrically connect a second side (cathode or anode) of the LEDs 801 (FIG. 8) to the substrate 1200. The connector end 1306 has a connector 1530 with connector pads 1532, 1534 that mount and electrically connect the emitter assembly 500 (FIG. 23), including the substrate 1200, to the flex circuit 2200 (FIG. 22). Substrate layers 1401-1406 (FIG. 14) have traces that electrically connect the component pads 1510 and wire bond pads 1520 to the connector 1532-1534. A thermistor 1540 is mounted to thermistor pads 1550 at the component end 1305, which are also electrically connected with traces to the connector 1530. Plated thru holes electrically connect the connector pads 1532, 1534 on the component and solder sides 1301, 1302, respectively.

[0045] FIG. 17 illustrates the electrical layout of a substrate 1200. A portion of the LEDs 801, including D1-D4 and D13-D16 have cathodes physically and electrically connected to component pads 1510 (FIG. 15) and corresponding anodes wire bonded to wire bond pads 1520. Another portion of the LEDs 801, including D5-D8 and D9-D12, have anodes physically and electrically connected to component pads 1510 (FIG. 15) and corresponding cathodes wire bonded to wire bond pads 1520. The connector 1530 has row pinouts J21-J24, column pinouts J31-J34 and thermistor pinouts J40-J41 for the LEDs 801 and thermistor 1540.

#### Interconnect Assembly

[0046] FIG. 19 illustrates an interconnect assembly

1900 that mounts the emitter assembly 500 and detector assembly 2400, connects to the sensor cable 4400 and provides electrical communications between the cable and each of the emitter assembly 500 and detector assembly 2400. The

interconnect assembly 1900 is incorporated with the attachment assembly 2700, which holds the emitter and detector assemblies to a tissue site. An interconnect assembly utilizing a flexible (flex) circuit is described with respect to FIGS. 20-24, below.

[0047] FIG. 20 illustrates an Interconnect assembly 1900 having a circuit substrate 2200, an emitter mount 2210, a detector mount 2220 and a cable connector 2230. The emitter mount 2210, detector mount 2220 and cable connector 2230 are disposed on the circuit substrate 2200. The emitter mount 2210 is adapted to mount an emitter assembly 500 having multiple emitters. The detector mount 2220 is adapted to mount a detector assembly 2400 having a detector. The cable connector 2230 is adapted to attach a sensor cable 4400. A first plurality of conductors 2040 disposed on the circuit substrate 2200 electrically interconnects the emitter mount 2210 and the cable connector 2230. A second plurality of conductors 2050 disposed on the circuit substrate 2200 electrically interconnects the detector mount 2220 and the cable connector 2230. A decoupling 2060 disposed proximate the cable connector 2230 substantially mechanically isolates the cable connector 2230 from both the emitter mount 2210 and the detector mount 2220 so that sensor cable stiffness is not translated to the emitter assembly 500 or the detector assembly 2400. A shield 2070 is adapted to fold over and shield one or more wires or pairs of wires of the sensor cable 4400.

[0048] FIG. 21 illustrates a flex circuit assembly 1900 having a flex circuit 2200, an emitter assembly 500 and a detector assembly 2400, which is configured to terminate the sensor end of a sensor cable 4400. The flex circuit assembly 1900 advantageously provides a structure that electrically connects yet mechanically isolates the sensor cable 4400, the emitter assembly 500 and the detector assembly 2400. As a result, the mechanical stiffness of the sensor cable 4400 is not translated to the sensor pads 3000, 3100 (FIGS. 30-31), allowing a comfortable finger attachment for the sensor 200 (FIG. 1). In particular, the emitter assembly 500 and detector assembly 2400 are mounted to opposite ends 2201, 2202 (FIG. 22) of an elongated flex circuit 2200. The sensor cable 4400 is mounted to a cable connector 2230 extending from a middle portion of the flex circuit 2200. Detector wires 4470 are shielded at the flex circuit junction by a fold-over conductive ink flap 2240, which is connected to a cable inner shield 4450. The flex circuit 2200 is described in further detail with respect to FIG. 22. The emitter portion of the flex circuit assembly 1900 is described in further detail with respect to FIG. 23. The detector assembly 2400 is described with respect to FIG. 24. The sensor cable 4400 is described with respect to FIGS. 44A-B, below.

[0049] FIG. 22 illustrates a sensor flex circuit 2200 having an emitter end 2201, a detector end 2202, an elongated interconnect 2204, 2206 between the ends 2201, 2202 and a cable connector 2230 extending from the interconnect 2204, 2206. The emitter end 2201 forms a "head" having emitter solder pads 2210 for attaching the emitter assembly 500 (FIG. 6) and mounting ears 2214 for attaching to the emitter pad 3000 (FIG. 30B), as described below. The detector end 2202 has detector solder pads for attaching the detector 2410 (FIG. 24). The interconnect 2204 between the emitter end 2201 and the cable connector 2230 forms a "neck," and the interconnect 2206 between the detector end 2202 and the cable connector 2230 forms a "tail." The cable connector 2230 forms "wings" that extend from the interconnect 2204, 2206 between the neck 2204 and tail 2206. A conductive ink flap 2240 connects to the cable inner shield 4450 (FIGS. 44A-B) and folds over to shield the detector wires 4470 (FIGS. 44A-B) soldered to the detector wire pads 2236. The outer wire pads 2238 connect to the remaining cable wires 4430 (FIGS. 44A-B). The flex circuit 2200 has top coverlay, top ink, inner coverlay, trace, trace base, bottom ink and bottom coverlay layers.

[0050] The flex circuit 2200 advantageously provides a connection between a multiple wire sensor cable 4400 (FIGS. 44A-B), a multiple wavelength emitter assembly 500 (FIG. 6) and a detector assembly 2400 (FIG. 24) without rendering the emitter and detector assemblies unwieldy and stiff. In particular, the wings 2230 provide a relatively large solder pad area 2232 that is narrowed at the neck 2204 and tail 2206 to mechanically isolate the cable 4400 (FIGS. 44A-B) from the remainder of the flex circuit 2200. Further, the neck 2206 is folded (see FIG. 4) for installation in the emitter pad 3000 (FIGS. 30A-H) and acts as a flexible spring to further mechanically isolate the cable 4400 (FIGS. 44A-B) from the emitter assembly 500 (FIG. 4). The tail 2206 provides an integrated connectivity path between the detector assembly 2400 (FIG. 24) mounted in the detector pad 3100 (FIGS. 31A-H) and the cable connector 2230 mounted in the opposite emitter pad 3000 (FIGS. 30A-H).

[0051] FIG. 23 illustrates the emitter portion of the flex circuit assembly 1900 (FIG. 21) having the emitter assembly 500. The emitter assembly connector 1530 is attached to the emitter end 2210 of the flex circuit 2200 (FIG. 22). In particular, reflow solder 2330 connects thru hole pads 1532, 1534 of the emitter assembly 500 to corresponding emitter pads 2310 of the flex circuit 2200 (FIG. 22).

[0052] FIG. 24 illustrates a detector assembly 2400 including a detector 2410, solder pads 2420, copper mesh tape 2430, an EMI shield 2440 and foil 2450. The detector 2410 is soldered 2460 chip side down to detector solder pads 2420 of the flex circuit 2200. The detector solder joint and detector ground pads 2420 are wrapped with the Kapton tape 2470. EMI shield tabs 2442 are folded onto the detector pads 2420 and soldered. The EMI shield walls are folded around the detector 2410 and the

remaining tabs 2442 are soldered to the back of the EMI shield 2440. The copper mesh tape 2430 is cut to size and the shielded detector and flex circuit solder joint are wrapped with the copper mesh tape 2430. The foil 2450 is cut to size with a predetermined aperture 2452. The foil 2450 is wrapped around shielded detector with the foil side in and the aperture 2452 is aligned with the EMI shield grid 2444.

#### 10 Detector Assembly

[0053] FIG. 25 illustrates an alternative detector assembly 2400 having adjacent detectors. Optical radiation having multiple wavelengths generated by emitters 700 is transmitted into a tissue site 1. Optical radiation at a first set of wavelengths is detected by a first detector 2510, such as, for example, a Si detector. Optical radiation at a second set of wavelengths is detected by a second detector 2520, such as, for example, a GaAs detector.

[0054] FIG. 26 illustrates another alternative detector assembly 2400

having stacked detectors coaxial along a light path. Optical radiation having multiple wavelengths generated by emitters 700 is transmitted into a tissue site 1. Optical radiation at a first set of wavelengths is detected by a first detector 2610. Optical radiation at a second set of wavelengths passes through the first detector 2610 and is detected by a second detector 2620.

A silicon (Si) detector and a gallium arsenide (GaAs) detector can be used. The Si detector is placed on top of the GaAs detector so that light must pass through the Si detector before reaching the GaAs detector. The Si detector can be placed directly on top of the GaAs detector or the Si and GaAs detector can be separated by some other medium, such as a transparent medium or air. A germanium detector may be used

instead of the GaAs detector. Advantageously, the stacked detector arrangement minimizes error caused by pathlength differences as compared with the adjacent detector.

#### Finger Clip

[0055] FIG. 27 illustrates a finger clip 2700 of a physiological sensor attachment assembly. The finger clip 2700 is configured to removably attach an emitter assembly 500 (FIG. 6) and detector assembly 2400 (FIG. 24), interconnected by a flex circuit assembly 1900, to a fingertip. The finger clip 2700 has an emitter shell 3800, an emitter pad 3000, a detector pad 2800 and a detector shell 3900. The emitter shell 3800 and the detector shell 3900 are rotatably connected and urged together by the spring assembly 3500. The emitter pad 3000 is fixedly retained by the emitter shell. The emitter assembly 500 (FIG. 6) is mounted proximate the emitter pad 3000 and adapted to transmit optical radiation having a plurality of wavelengths into fingertip tissue. The detector pad 2800

is fixedly retained by the detector shell **3900**. The detector assembly **3500** is mounted proximate the detector pad **2800** and adapted to receive the optical radiation after attenuation by fingertip tissue.

[0056] FIG. **28** illustrates a detector pad **2800** advantageously configured to position and comfortably maintain a fingertip relative to a detector assembly for accurate sensor measurements. In particular, the detector pad has fingertip positioning features including a guide **2810**, a contour **2820** and a stop **2830**. The guide **2810** is raised from the pad surface **2803** and narrows as the guide **2810** extends from a first end **2801** to a second end **2802** so as to increasingly conform to a fingertip as a fingertip is inserted along the pad surface **2803** from the first end **2801**. The contour **2820** has an indentation defined along the pad surface **2803** generally shaped to conform to a fingertip positioned over a detector aperture **2840** located within the contour **2820**. The stop **2830** is raised from the pad surface **2803** so as to block the end of a finger from inserting beyond the second end **2802**. FIGS. **29A-B** illustrate detector pads **3100**, **3400** each having a guide **2810**, a contour **2820** and a stop **2830**, described in further detail with respect to FIGS. **31** and **34**, respectively.

[0057] FIGS. **30A-H** illustrate an emitter pad **3000** having emitter pad flaps **3010**, an emitter window **3020**, mounting pins **3030**, an emitter assembly cavity **3040**, isolation notches **3050**, a flex circuit notch **3070** and a cable notch **3080**. The emitter pad flaps **3010** overlap with detector pad flaps **3110** (FIGS. **31A-H**) to block ambient light. The emitter window **3020** provides an optical path from the emitter array **700** (FIG. **8**) to a tissue site. The mounting pins **3030** accommodate apertures in the flex circuit mounting ears **2214** (FIG. **22**), and the cavity **3040** accommodates the emitter assembly **500** (FIG. **21**). Isolation notches **3050** mechanically decouple the shell attachment **3060** from the remainder of the emitter pad **3000**. The flex circuit notch **3070** accommodates the flex circuit tail **2206** (FIG. **22**) routed to the detector pad **3100** (FIGS. **31A-H**). The cable notch **3080** accommodates the sensor cable **4400** (FIGS. **44A-B**). FIGS. **33A-H** illustrate an alternative slim finger emitter pad **3300**.

[0058] FIGS. **31A-H** illustrate a detector pad **3100** having detector pad flaps **3110**, a shoe box cavity **3120** and isolation notches **3150**. The detector pad flaps **3110** overlap with emitter pad flaps **3010** (FIGS. **30A-H**), interleaving to block ambient light. The shoe box cavity **3120** accommodates a shoe box **3200** (FIG. **32A-H**) described below. Isolation notches **3150** mechanically decouple the attachment points **3160** from the remainder of the detector pad **3100**. FIGS. **34A-H** illustrate an alternative slim finger detector pad **3400**.

[0059] FIGS. **32A-H** illustrate a shoe box **3200** that accommodates the detector assembly **2400** (FIG. **24**). A detector window **3210** provides an optical path from a tissue site to the detector **2410** (FIG. **24**). A flex circuit notch **3220** accommodates the flex circuit tail **2206** (FIG. **22**) routed from the emitter pad **3000** (FIGS. **30A-H**). The shoe box **3200** may be colored black or other substan-

tially light absorbing color and the emitter pad **3000** and detector pad **3100** are each colored white or other substantially light reflecting color.

[0060] FIGS. **35-37** illustrate a spring assembly **3500** having a spring **3600** configured to urge together an emitter shell **3800** (FIG. **46**) and a detector shell **3900**. The detector shell is rotatably connected to the emitter shell. The spring is disposed between the shells **3800**, **3900** and adapted to create a pivot point along a finger gripped between the shells that is substantially behind the fingertip. This advantageously allows the shell hinge **3810**, **3910** (FIGS. **38-39**) to expand so as to distribute finger clip force along the inserted finger, comfortably keeping the fingertip in position over the detector without excessive force.

[0061] As shown in FIGS. **36A-C**, the spring **3600** has coils **3610**, an emitter shell leg **3620** and a detector shell leg **3630**. The emitter shell leg **3620** presses against the emitter shell **3800** (FIGS. **38A-D**) proximate a grip **3820** (FIGS. **38A-D**). The detector shell legs **3630** extend along the detector shell **3900** (FIGS. **39A-D**) to a spring plate **3700** (FIGS. **37A-D**) attachment point. The coil **3610** is secured by hinge pins **410** (FIG. **46**) and is configured to wind as the finger clip is opened, reducing its diameter and stress accordingly.

[0062] As shown in FIGS. **37A-D** the spring plate **3700** has attachment apertures **3710**, spring leg slots **3720**, and a shelf **3730**. The attachment apertures **3710** accept corresponding shell posts **3930** (FIGS. **39A-D**) so as to secure the spring plate **3700** to the detector shell **3900** (FIG. **39A-D**). Spring legs **3630** (FIG. **36A-C**) are slidably anchored to the detector shell **3900** (FIG. **39A-D**) by the shelf **3730**, advantageously allowing the combination of spring **3600**, shells **3800**, **3900** and hinges **3810**, **3910** to adjust to various finger-sizes and shapes.

[0063] FIGS. **38-39** illustrate the emitter and detector shells **3800**, **3900**, respectively, having hinges **3810**, **3910** and grips **3820**, **3920**. Hinge apertures **3812**, **3912** accept hinge pins **410** (FIG. **46**) so as to create a finger clip. The detector shell hinge aperture **3912** is elongated, allowing the hinge to expand to accommodate a finger.

#### Monitor And Sensor

[0064] FIG. **40** illustrates a monitor **100** and a corresponding sensor assembly **200**, as described generally with respect to FIGS. **1-3**, above. The sensor assembly **200** has a sensor **400** and a sensor cable **4400**. The sensor **400** houses an emitter assembly **500** having emitters responsive to drivers within a sensor controller **4500** so as to transmit optical radiation into a tissue site. The sensor **400** also houses a detector assembly **2400** that provides a sensor signal **2500** responsive to the optical radiation after tissue attenuation. The sensor signal **2500** is filtered, amplified, sampled and digitized by the front-end **4030** and input to a DSP (digital signal processor) **4040**, which also commands the sensor controller **4500**. The sensor cable **4400** electrically communicates drive

signals from the sensor controller **4500** to the emitter assembly **500** and a sensor signal **2500** from the detector assembly **2400** to the front-end **4030**. The sensor cable **4400** has a monitor connector **210** that plugs into a monitor sensor port **110**.

[0065] The monitor **100** also may have a reader **4020** capable of obtaining information from an information element (IE) in the sensor assembly **200** and transferring that information to the DSP **4040**, to another processor or component within the monitor **100**, or to an external component or device that is at least temporarily in communication with the monitor **100**.

The reader function is preferably incorporated within the DSP **4040**, utilizing one or more of DSP I/O, ADC, DAC features and corresponding processing routines, as examples.

[0066] The monitor connector **210** preferably houses the information element **4000**, which may be a memory device or other active or passive electrical component. The information element **4000** may be an EPROM, or other programmable memory, or an EEPROM, or other reprogrammable memory, or both. The information element **4000** is preferably housed within the sensor **400**, or an information element **4000** is housed within both the monitor connector **4000** and the sensor **400**. The emitter assembly **500** preferably has an information element **4000**, which is read in response to one or more drive signals from the sensor controller **4500**, as described with respect to FIGS. **41-43**, below.

A memory information element may be incorporated into the emitter array **700** (FIG. **8**) and has characterization information relating to the LEDs **801** (FIG. **8**). Trend data relating to slowly varying parameters, such as perfusion index, HbCO or METHb, to name a few, are preferably stored in an IE memory device, such as EEPROM.

#### Back-to-Back LEDs

[0067] FIGS. **41-43** illustrate alternative sensors. A sensor controller **4500** configured to activate an emitter array **700** (FIG. **7**) arranged in an electrical grid, is described with respect to FIG. **7**, above. Advantageously, a sensor controller **4500** so configured is also capable of driving a conventional two-wavelength (red and IR) sensor **4100** having back-to-back LEDs **4110**, **4120** or an information element **4300** or both.

[0068] FIG. **41A** illustrates a sensor **4100** having an electrical grid **4130** configured to activate light emitting sources by addressing at least one row conductor and at least one column conductor. A first LED **4110** and a second LED **4120** are configured in a back-to-back arrangement so that a first contact **4152** is connected to a first LED **4110** cathode and a second LED **4120** anode and a second contact **4154** is connected to a first LED **4110** anode and a second LED **4120** cathode. The first contact **4152** is in communications with a first row conductor **4132** and a first column conductor **4134**. The sec-

ond contact is in communications with a second row conductor **4136** and a second column conductor **4138**. The first LED **4110** is activated by addressing the first row conductor **4132** and the second column conductor **4138**.

5 The second LED **4120** is activated by addressing the second row conductor **4136** and the first column conductor **4134**.

[0069] FIG. **41B** illustrates a sensor cable **4400** capable of communicating signals between a monitor **100** and a sensor **4100**. The cable **4400** has a first row input **4132**, a first column input **4134**, a second row input **4136** and a second column input **4138**. A first output **4152** combines the first row input **4132** and the first column input **4134**. A second output **4154** combines a second row input **4136** and second column input **4138**.

[0070] FIG. **41C** illustrates a monitor **100** capable of communicating drive signals to a sensor **4100**. The monitor **4400** has a first row signal **4132**, a first column signal **4134**, a second row signal **4136** and a second column signal **4138**. A first output signal **4152** combines the first row signal **4132** and the first column signal **4134**. A second output signal **4154** combines a second row signal **4136** and second column signal **4138**.

#### Information Elements

[0071] FIGS. **42-43** illustrate information elements **4200-4300** in communications with emitter array drivers configured to activate light emitters connected in an electrical grid. The information elements are configured to provide information as DC values, AC values or a combination of DC and AC values in response corresponding DC, AC or combination DC and AC electrical grid drive signals. FIG. **42** illustrates information element **4200** advantageously driven directly by an electrical grid having rows **710** and columns **720**. In particular, the information element **4200** has a series connected resistor  $R_2$  **4210** and diode **4220** connected between a row line **710** and a column line **720** of an electrical grid. In this manner, the resistor  $R_2$  value can be read in a similar manner that LEDs **810** (FIG. **8**) are activated. The diode **4220** is oriented, e.g. anode to row and cathode to column as the LEDs so as to prevent parasitic currents from unwanted activation of LEDs **810** (FIG. **8**).

[0072] FIGS. **43A-C** illustrate other embodiments where the value of  $R_1$  is read with a DC grid drive current and a corresponding grid output voltage level.

The combined values of  $R_1$ ,  $R_2$  and  $C$  or, alternatively,  $R_1$ ,  $R_2$  and  $L$  may be read with a varying (AC) grid drive currents and a corresponding grid output voltage waveform. As one example, a step in grid drive current is used to determine component values from the time constant of a corresponding rise in grid voltage. As another example, a sinusoidal grid drive current is used to determine component values from the magnitude or phase or both of a corresponding sinusoidal grid voltage. The component values determined by DC or AC electrical grid drive currents can represent sensor types, authorized suppli-

ers or manufacturers, emitter wavelengths among others. Further, a diode D (FIG. 43C) can be used to provide one information element reading  $R_1$  at one drive level or polarity and another information element reading, combining  $R_1$  and  $R_2$ , at a second drive level or polarity, i.e. when the diode is forward biased.

[0073] Passive information element 4300 may include any of various combinations of resistors, capacitors or inductors connected in series and parallel, for example. Other information element 4300

connected to an electrical grid and read utilizing emitter array drivers incorporate other passive components, active components or memory components, alone or in combination, including transistor networks, PROMs, ROMs, EPROMs, EEPROMs, gate arrays and PLAs to name a few.

#### Sensor Cable

[0074] FIGS. 44A-B illustrate a sensor cable 4400 having an outer jacket 4410, an outer shield 4420, multiple outer wires 4430, an inner jacket 4440, an inner shield 4450, a conductive polymer 4460 and an inner twisted wire pair 4470. The outer wires 4430 are advantageously configured to compactly carry multiple drive signals to the emitter array 700 (FIG. 7). There may be twelve outer wires 4430 corresponding to four anode drive signals 4501 (FIG. 45), four cathode drive signals 4502 (FIG. 45), two thermistor pinouts 1450 (FIG. 15) and two spares. The inner twisted wire pair 4470 corresponds to the sensor signal 2500 (FIG. 25) and is extruded within the conductive polymer 4460 so as to reduce triboelectric noise. The shields 4420, 4450 and the twisted pair 4470 boost EMI and crosstalk immunity for the sensor signal 2500 (FIG. 25).

#### Controller

[0075] FIG. 45 illustrates a sensor controller 4500 located in the monitor 100 (FIG. 1) and configured to provide anode drive signals 4501 and cathode drive signals 4502 to the emitter array 700 (FIG. 7). The DSP (digital signal processor) 4040, which performs signal processing functions for the monitor, also provides commands 4042 to the sensor controller 4500. These commands determine drive signal 4501, 4502 levels and timing. The sensor controller 4500 has a command register 4510, an anode selector 4520, anode drivers 4530, current DACs (digital-to-analog converters) 4540, a current multiplexer 4550, cathode drivers 4560, a current meter 4570 and a current limiter 4580. The command register 4510 provides control signals responsive to the DSP commands 4042.

The command register 4510 may be a shift register that loads serial command data 4042 from the DSP 4040 and synchronously sets output bits that select or enable various functions within the sensor controller 4500, as described below.

[0076] As shown in FIG. 45, the anode selector 4520 is responsive to anode select 4516 inputs from the command register 4510 that determine which emitter array row 810 (FIG. 8) is active. Accordingly, the anode selector 4520 sets one of the anode on 4522 outputs to the anode drivers 4530, which pulls up to  $V_{cc}$  one of the anode outputs 4501 to the emitter array 700 (FIG. 8).

[0077] Also shown in FIG. 45, the current DACs 4540 are responsive to command register data 4519 that determines the currents through each emitter array column 820 (FIG. 8). There are preferably four, 12-bit DACs associated with each emitter array column 820 (FIG. 8), sixteen DACs in total. That is, there are four DAC outputs 4542 associated with each emitter array column 820 (FIG. 8) corresponding to the currents associated with each row 810 (FIG. 8) along that column 820 (FIG. 8). All sixteen DACs 4540 can be organized as a single shift register, and the command register 4510 serially clocks DAC data 4519 into the DACs 4540. A current multiplexer 4550 is responsive to cathode on 4518 inputs from the command register 4510 and anode on 4522 inputs from the anode selector 4520 so as to convert the appropriate DAC outputs 4542 to current set 4552 inputs to the cathode drivers 4560. The cathode drivers 4560 are responsive to the current set 4552 inputs to pull down to ground one to four of the cathode outputs 4502 to the emitter array 700 (FIG. 8).

[0078] The current meter 4570 outputs a current measure 4572 that indicates the total LED current driving the emitter array 700 (FIG. 8). The current limiter 4580 is responsive to the current measure 4572 and limits specified by the command register 4510 so as to prevent excessive power dissipation by the emitter array 700 (FIG. 8). The current limiter 4580 provides an enable 4582 output to the anode selector 4520. A Hi Limit 4512 input specifies the higher of two preset current limits. The current limiter 4580 latches the enable 4582 output in an off condition when the current limit is exceeded, disabling the anode selector 4520. A trip reset 4514 input resets the enable 4582 output to re-enable the anode selector 4520.

#### Sensor Assembly

[0079] As shown in FIG. 46, the sensor 400 has an emitter shell 3800, an emitter pad 3000, a flex circuit assembly 2200, a detector pad 3100 and a detector shell 3900. A sensor cable 4400 attaches to the flex circuit assembly 2200, which includes a flex circuit 2100, an emitter assembly 500 and a detector assembly 2400. The portion of the flex circuit assembly 2200 having the sensor cable 4400 attachment and emitter assembly 500 is housed by the emitter shell 3800 and emitter pad 3000. The portion of the flex circuit assembly 2200 having the detector assembly 2400 is housed by the detector shell 3900 and detector pad 3100. In particular, the detector assembly 2400 inserts into a shoe 3200, and the shoe 3200 inserts into the detector pad 3100. The emitter shell

**3800** and detector shell **3900** are fastened by and rotate about hinge pins **410**, which insert through coils of a spring **3600**. The spring **3600** is held to the detector shell **3900** with a spring plate **3700**. A finger stop **450** attaches to the detector shell. A silicon adhesive **420** may be used to attach the pads **3000**, **3100** to the shells **3800**, **3900**, a silicon potting compound **430** is used to secure the emitter and detector assemblies **500**, **2400** within the pads **3000**, **3100**, and a cyanoacrylic adhesive **440** secures the sensor cable **4400** to the emitter shell **3800**.

**[0080]** A multiple wavelength sensor has been disclosed in detail in connection with various examples and embodiments. These embodiments in line with the present invention are defined by the features of the claims that follow.

One of ordinary skill in art will appreciate many variations and modifications.

## Claims

### 1. A physiological sensor comprising:

a plurality of light emitting sources (801), each light emitting source configured to activate by addressing at least one of a plurality of rows (720) and at least one of a plurality of columns (740) of an electrical grid, the light emitting sources configured to transmit light of a plurality of wavelengths into body tissue and clustered in rows of said grid and according to wavelength so as to minimize path length variations and facilitate equalization of light emission intensities; and  
a detector (2400) configured to be responsive to the transmitted light after attenuation by said body tissue.

### 2. The physiological sensor according to claim 1 wherein multiple ones of the light emitting sources are configured to transmit light of substantially the same wavelength, the multiple ones configured to be simultaneously activated by addressing one of the rows.

### 3. The physiological sensor according to claims 1 or 2 wherein the light emitting sources comprise LEDs and each of the LEDs comprise an anode in common with one of the rows and a cathode in common with one of the columns of said electrical grid so that driving one of the rows and one of the columns activates a unique one of the LEDs.

### 4. The physiological sensor according to claim 3 further comprising:

a plurality of row drivers in communication with the rows; and

a plurality of column drivers in communication with the columns,

wherein a selected row driver sources current to a corresponding row and selected column driver sinks current from a corresponding column so as to activate an addressed one of the LEDs.

### 5. The physiological sensor according to claim 4 wherein deselected ones of the row drivers pull corresponding rows to a low voltage and deselected ones of the column drivers pull corresponding columns to a high voltage so as to substantially block parasitic current from unaddressed ones of the LEDs.

### 6. The physiological sensor according to claim 1 wherein the light sources comprise up to 16 LEDs and wherein the electrical grid comprises four rows and four columns in communication with said up to sixteen of LEDs.

### 7. A physiological sensor method comprising:

sequentially addressing a plurality of light emitting sources using a plurality of conductors of an electrical grid so as to emit light having a plurality of wavelengths that when attenuated by body tissue is indicative of at least one physiological characteristic,  
wherein each of the plurality of light emitting sources is configured to activate by addressing at least one of a plurality of rows and at least one of a plurality of columns of an electrical grid, and  
wherein the plurality of light emitting sources are clustered in rows of said electrical grid according to wavelength so as to minimize path length variations and facilitate equalization of light emission intensities; and  
detecting the emitted light after attenuation by body tissue.

### 8. The method according to claim 7 further comprising connecting one of each of the light emitting sources at a unique junction of the electrical grid.

### 9. The method according to claim 7 or 8 further comprising:

addressing a row one of the conductors; and  
addressing a column one of the conductors,  
wherein the light emitting source connected between the addressed row and the addressed column is activated.

### 10. The method according to claim 7 further comprising:

providing a plurality of same wavelength ones

of the light emitting sources; and simultaneously addressing substantially the same wavelength light emitting sources.

## Patentansprüche

### 1. Physiologischer Sensor, der aufweist:

mehrere lichtemittierende Quellen (801), wobei jede lichtemittierende Quelle konfiguriert ist, durch Adressieren mindestens einer von mehreren Reihen (720) und mindestens einer von mehreren Spalten (740) eines elektrischen Gitters zu aktivieren, wobei die lichtemittierenden Quellen konfiguriert sind, Licht mit mehreren Wellenlängen in Körpergewebe zu senden und in Reihen des Gitters und entsprechend der Wellenlänge angehäuft sind, um Weglängenvariationen zu minimieren und die Angleichung der Lichtemissionsintensitäten zu erleichtern; und einen Detektor (2400), der konfiguriert ist, auf das gesendete Licht nach einer Dämpfung durch das Körpergewebe zu reagieren.

### 2. Physiologischer Sensor nach Anspruch 1, wobei mehrere der lichtemittierenden Quellen konfiguriert sind, Licht mit im Wesentlichen derselben Wellenlänge zu senden, und die mehreren Quellen konfiguriert sind, durch Adressieren von einer der Reihen gleichzeitig aktiviert zu werden.

### 3. Physiologischer Sensor nach Anspruch 1 oder 2, wobei die lichtemittierenden Quellen LEDs aufweisen und jede der LEDs eine mit einer der Reihen gemeinsame Anode und eine mit einer der Spalten des elektrischen Gitters gemeinsame Kathode aufweist, so dass das Ansteuern von einer der Reihen und einer der Spalten eine einzige der LEDs aktiviert.

### 4. Physiologischer Sensor nach Anspruch 3, der ferner aufweist:

mehrere Reihentreiber in Verbindung mit den Reihen; und  
mehrere Spaltentreiber in Verbindung mit den Spalten,  
wobei ein ausgewählter Reihentreiber Strom zu einer entsprechenden Reihe leitet und ausgewählter Spaltentreiber Strom von einer entsprechenden Spalte ableitet, um eine adressierte der LEDs zu aktivieren.

### 5. Physiologischer Sensor nach Anspruch 4, wobei abgewählte der Reihentreiber entsprechende Reihen auf eine niedrige Spannung ziehen und abgewählte der Spaltentreiber entsprechende Spalten auf eine hohe Spannung ziehen, um einen parasitären Strom

von nicht adressierten der LEDs zu sperren.

### 6. Physiologischer Sensor nach Anspruch 1, wobei die Lichtquellen bis zu 16 LEDs aufweisen und wobei das elektrische Gitter vier Reihen und vier Spalten in Verbindung mit den bis zu sechzehn LEDs aufweisen.

### 7. Physiologisches Sensorverfahren, das aufweist:

sequentielles Adressieren von mehreren lichtemittierenden Quellen mittels mehrerer Leiter eines elektrischen Gitters, um Licht mit mehreren Wellenlängen zu emittieren, das, wenn es durch Körpergewebe gedämpft wird, mindestens eine physiologische Eigenschaft anzeigt, wobei jede der mehreren lichtemittierenden Quellen konfiguriert ist, durch Adressieren mindestens einer von mehreren Reihen und mindestens einer von mehreren Spalten eines elektrischen Gitters zu aktivieren, und wobei die mehreren lichtemittierenden Quellen in Reihen des Gitters entsprechend der Wellenlänge angehäuft sind, um Weglängenvariationen zu minimieren und die Angleichung der Lichtemissionsintensitäten zu erleichtern; und Detektieren des emittierten Lichts nach der Dämpfung durch Körpergewebe.

### 8. Verfahren nach Anspruch 7, das ferner das Anschließen von einer der lichtemittierenden Quellen an einer eindeutigen Verbindung des elektrischen Gitters aufweist.

### 9. Verfahren nach Anspruch 7 oder 8, das ferner aufweist:

Adressieren von einem der Leiter einer Reihe; und  
Adressieren von einem der Leiter einer Spalte, wobei die lichtemittierende Quelle, die zwischen die adressierte Reihe und die adressierte Spalte geschaltet ist, aktiviert wird.

### 10. Verfahren nach Anspruch 7, das ferner aufweist:

Bereitstellen von mehreren der lichtemittierenden Quellen mit derselben Wellenlänge; und im Wesentlichen gleichzeitiges Adressieren der lichtemittierenden Quellen mit derselben Wellenlänge.

## Revendications

### 1. Capteur physiologique, comprenant :

une pluralité de sources électroluminescentes

- (801),  
chaque source électroluminescente étant prévue pour  
activer par adressage au moins une rangée  
d'une pluralité de rangées (720) et au moins une  
colonne d'une pluralité de colonnes (740) d'un  
réseau électrique, les sources électrolumines-  
centes étant prévues pour transmettre la lumière  
d'une pluralité de longueurs d'onde dans le  
tissu corporel et étant regroupées en rangées  
dudit réseau en fonction de la longueur d'onde,  
de manière à minimiser les variations de lon-  
gueur de trajet et faciliter l'égalisation des inten-  
sités d'émission lumineuse ; et  
un détecteur (2400) prévu pour être réactif à la  
lumière transmise après atténuation par le tissu  
corporel.
2. Capteur physiologique selon la revendication 1, où  
plusieurs parmi les sources électroluminescentes  
sont prévues pour transmettre des lumières ayant  
sensiblement la même longueur d'onde, lesdites plu-  
sieurs sources étant prévues pour être activées si-  
multanément par adressage d'une des rangées.
  3. Capteur physiologique selon la revendication 1 ou  
la revendication 2, où les sources électrolumines-  
centes comprennent des LED et où chacune des  
LED comprend une anode en commun avec une des  
rangées et une cathode en commun avec une des  
colonnes du réseau électrique, de manière que la  
commande d'une des rangées et d'une des colonnes  
active une seule des LED.
  4. Capteur physiologique selon la revendication 3,  
comprenant en outre :  
  
une pluralité de pilotes de rangée en liaison avec  
les rangées ; et  
une pluralité de pilotes de colonne en liaison  
avec les colonnes,  
où un pilote de rangée sélectionné fournit un  
courant à une rangée correspondante et un pi-  
lote de colonne sélectionné affaiblit le courant  
d'une colonne correspondante de manière à ac-  
tiver une LED adressée parmi les LED.
  5. Capteur physiologique selon la revendication 4, où  
des pilotes désélectionnés parmi les pilotes de ran-  
gée tirent des rangées correspondantes  
vers une basse tension, et des pilotes désélection-  
nés parmi les pilotes de colonne tirent des colonnes  
correspondantes vers une haute tension, de maniè-  
re à bloquer sensiblement le courant parasite de LED  
non adressées parmi les LED.
  6. Capteur physiologique selon la revendication 1, où  
les sources lumineuses comprennent jusqu'à 16
- LED et où le réseau électrique comprend quatre ran-  
gées et quatre colonnes en liaison avec lesdites jus-  
qu'à 16 LED.
7. Procédé de capteur physiologique, comprenant :  
  
l'adressage séquentiel d'une pluralité de sour-  
ces électroluminescentes au moyen d'une plu-  
ralité de conducteurs d'un réseau électrique, de  
manière à émettre une lumière ayant une plu-  
ralité de longueurs d'onde, laquelle est indicati-  
ve d'au moins une caractéristique physiologi-  
que, quand elle est atténuée par le tissu corporel,  
où chaque source de la pluralité de sources  
électroluminescentes est prévue pour activer  
par adressage au moins une rangée d'une plu-  
ralité de rangées et au moins une colonne d'une  
pluralité de colonnes d'un réseau électrique, et  
où la pluralité de sources électroluminescentes  
sont regroupées en rangées du réseau électri-  
que en fonction de la longueur d'onde, de ma-  
nière à minimiser les variations de longueur de  
trajet et faciliter l'égalisation des intensités  
d'émission lumineuse ; et  
où la lumière émise est détectée après atténua-  
tion par le tissu corporel.
  8. Procédé selon la revendication 7, comprenant en  
outre la connexion de chacune des sources électro-  
luminescentes à une jonction unique du réseau élec-  
trique.
  9. Procédé selon la revendication 7 ou la revendication  
8, comprenant en outre :  
  
l'adressage d'une rangée par un des  
conducteurs ; et  
l'adressage d'une rangée par un des conduc-  
teurs,  
la source électroluminescente connectée entre  
la rangée adressée et la colonne adressée étant  
activée.
  10. Procédé selon la revendication 7, comprenant en  
outre :  
  
la préparation d'une pluralité de sources de mê-  
me longueur d'onde parmi les sources  
électroluminescentes ; et  
l'adressage simultané des sources électrolumi-  
nescentes ayant sensiblement la même lon-  
gueur d'onde.

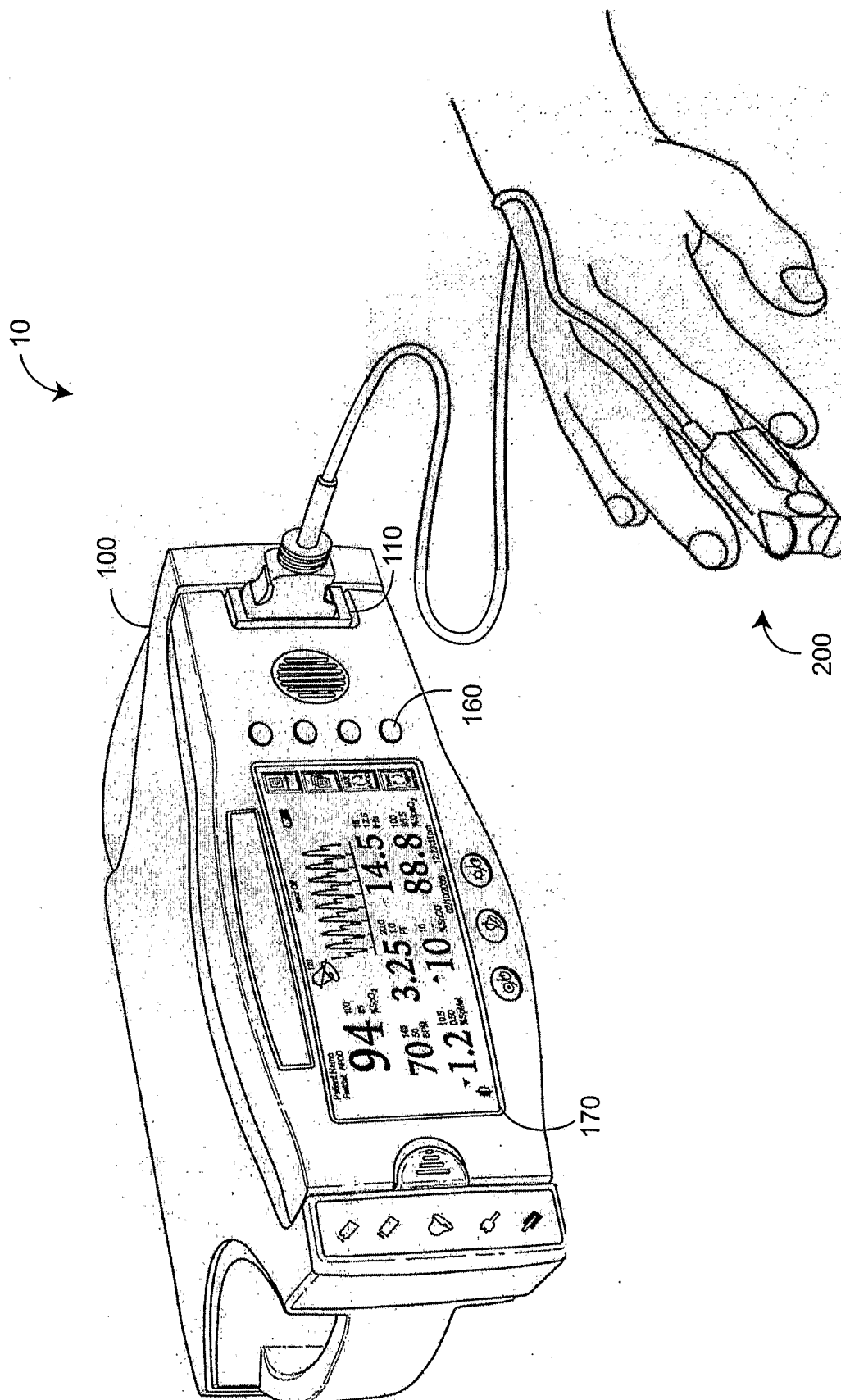


FIG. 1

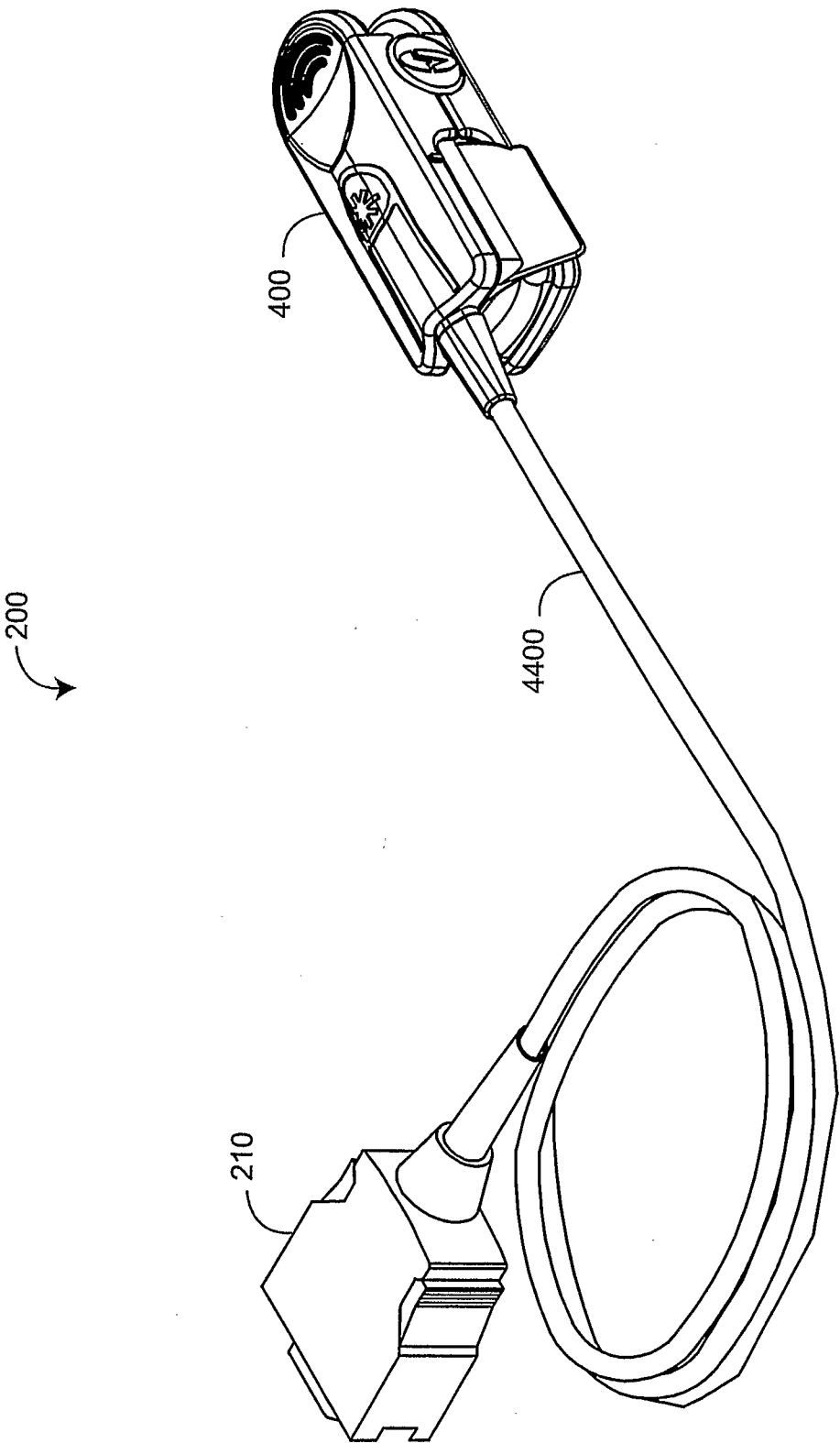


FIG. 2A

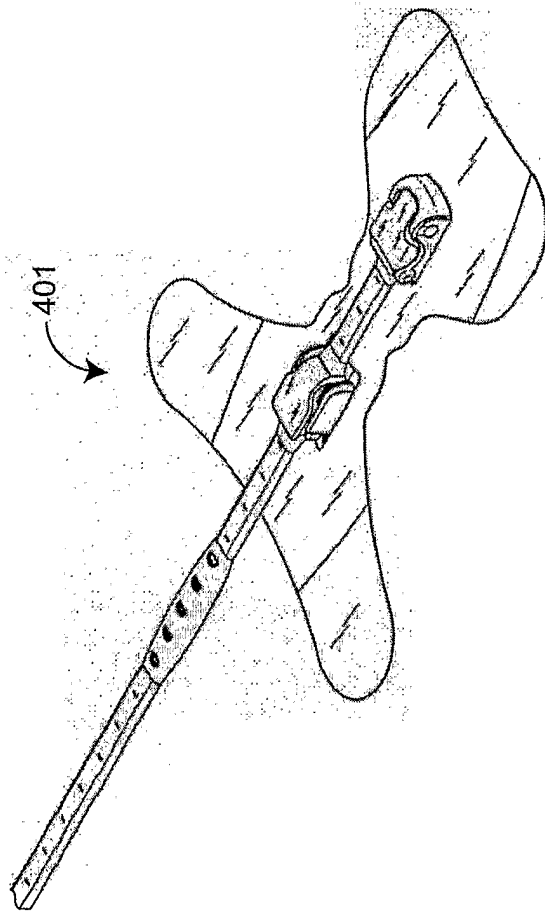


FIG. 2B

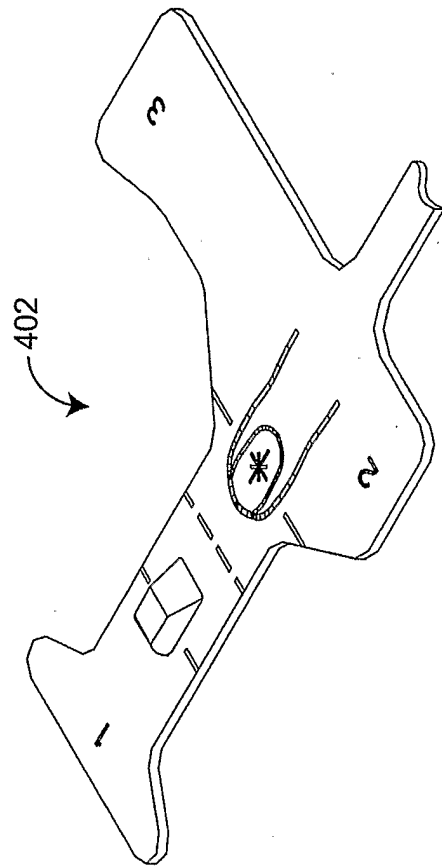


FIG. 2C

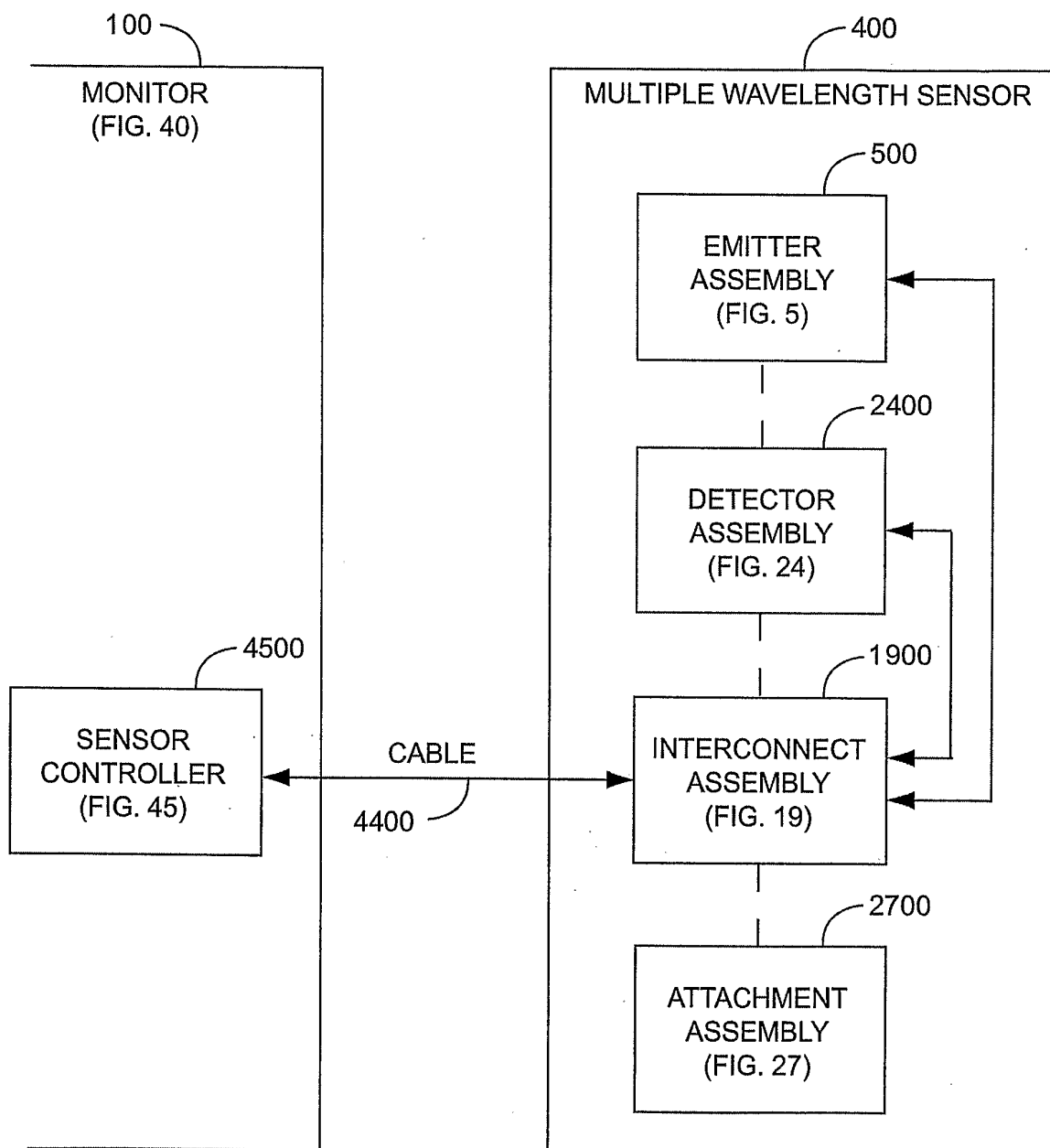


FIG. 3

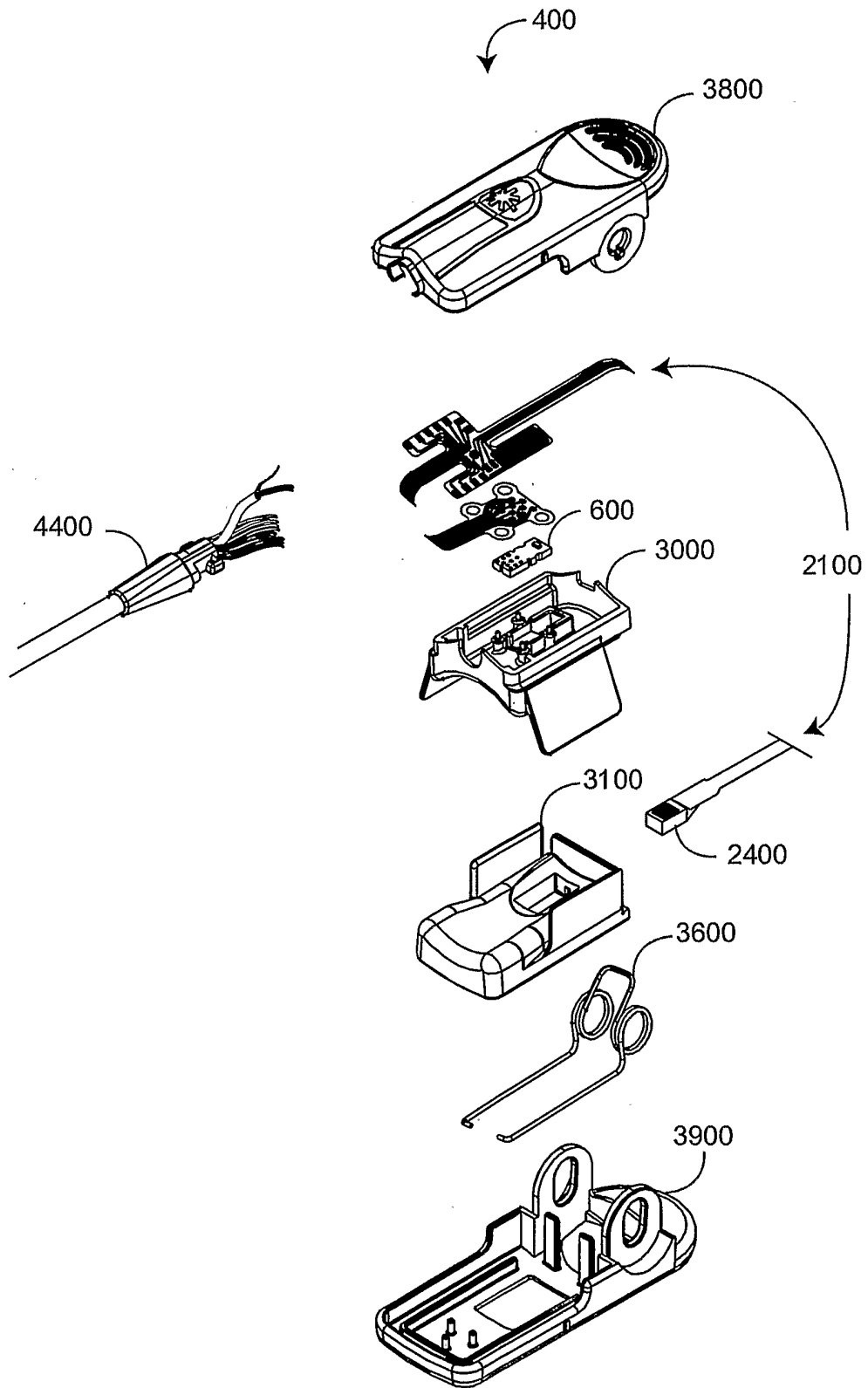


FIG. 4

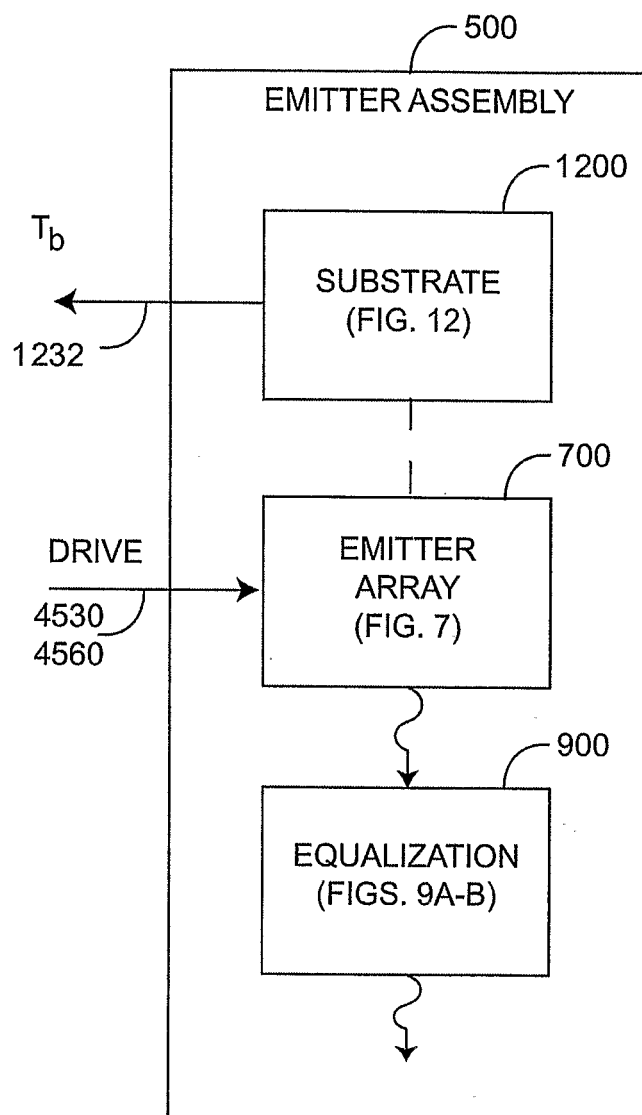


FIG. 5

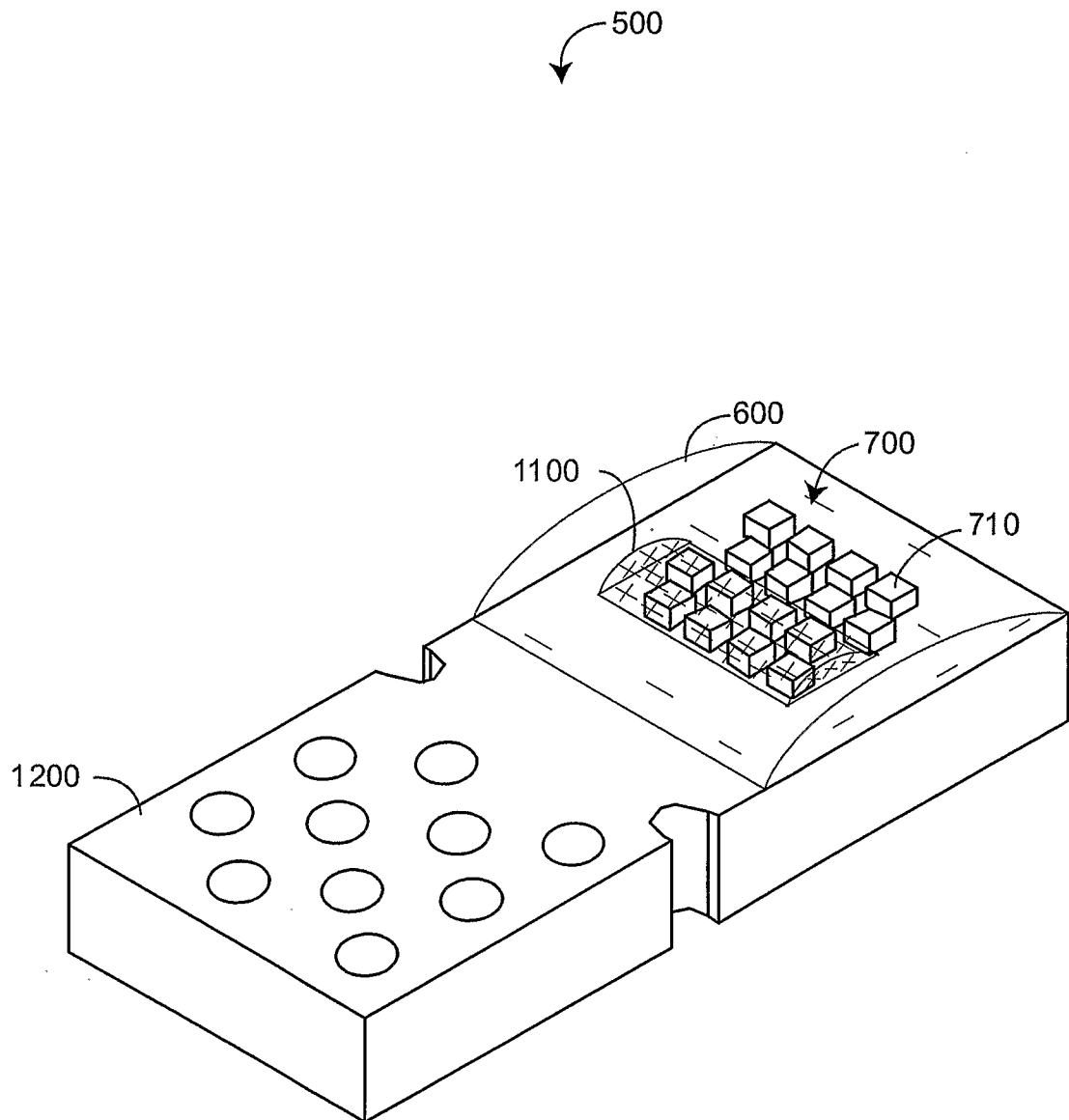


FIG. 6

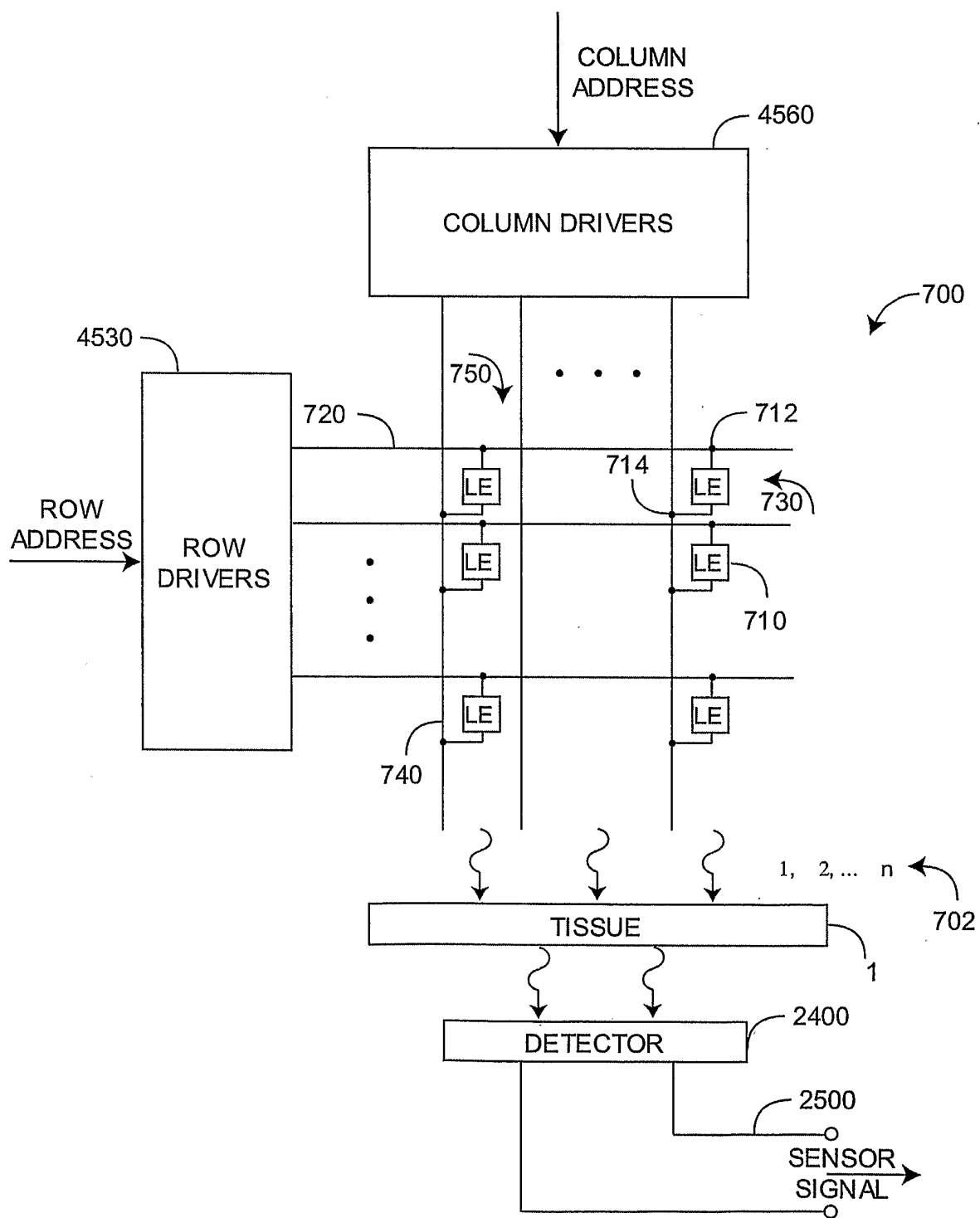


FIG. 7

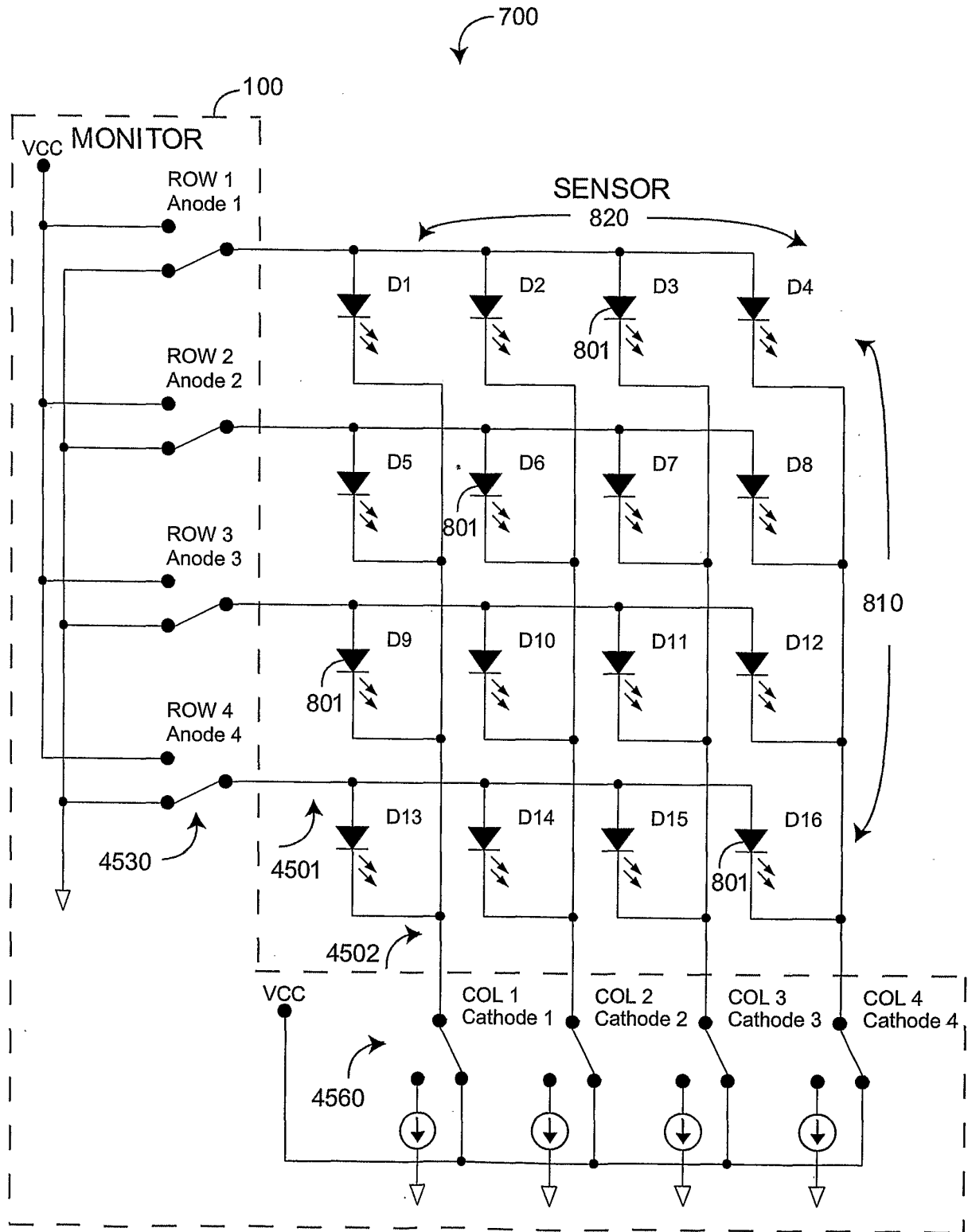


FIG. 8

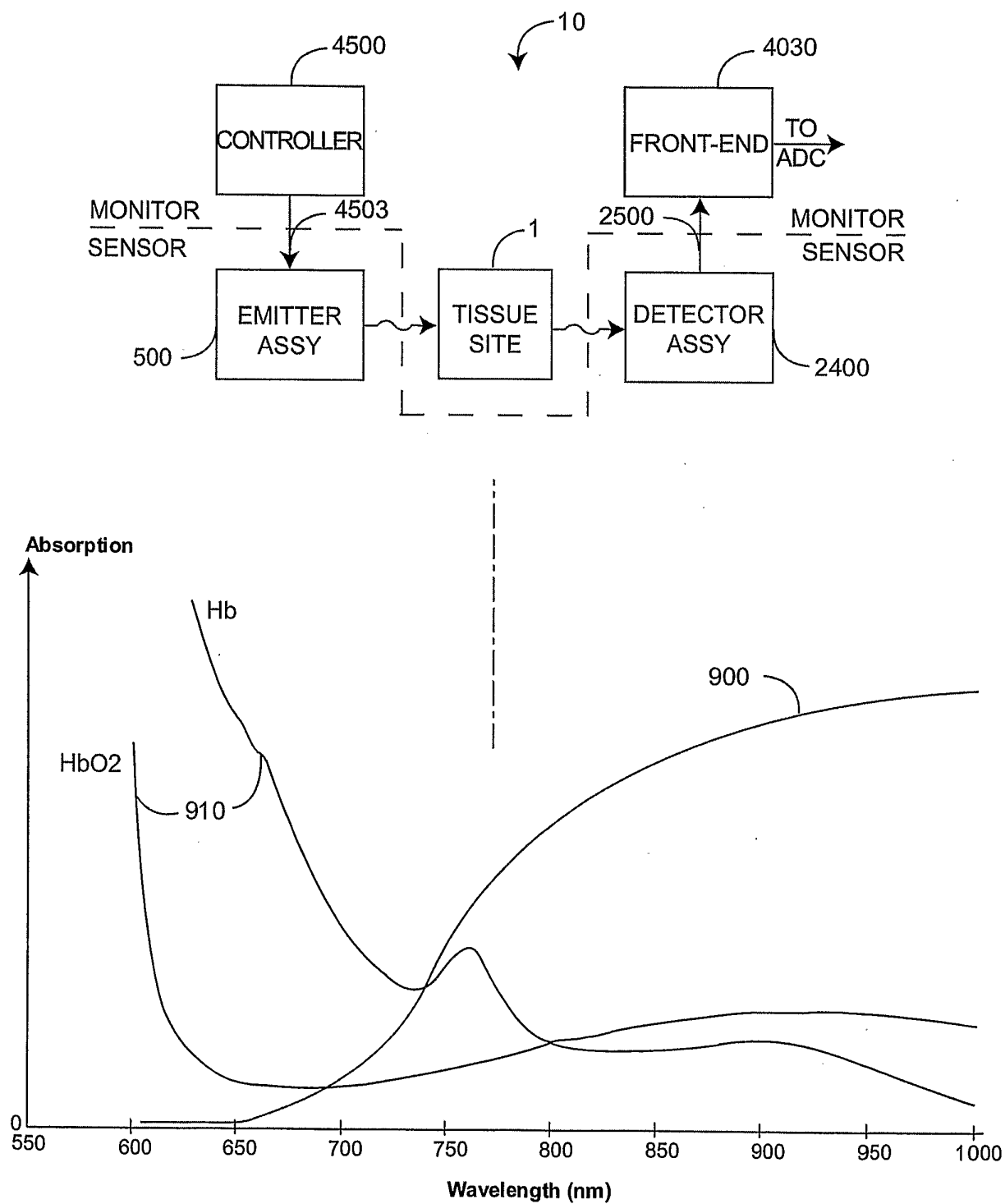


FIG. 9

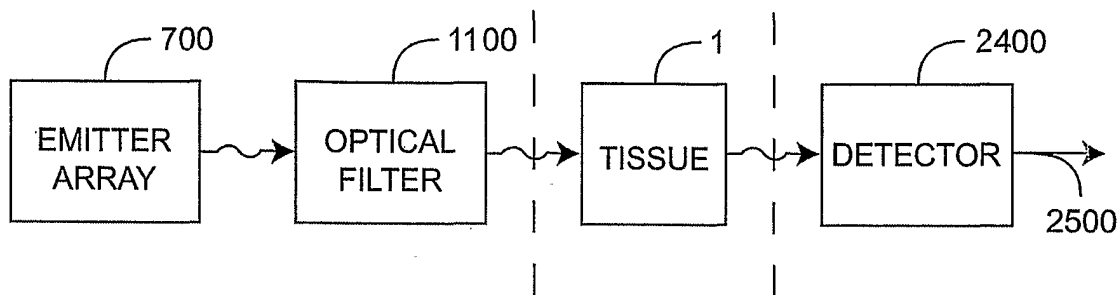


FIG. 10A

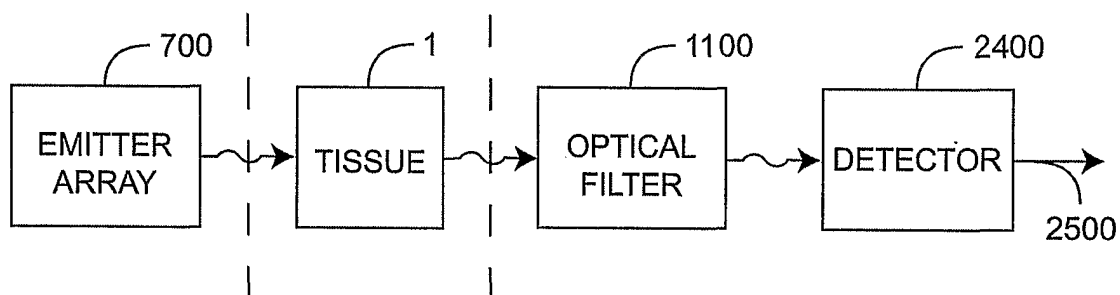


FIG. 10B

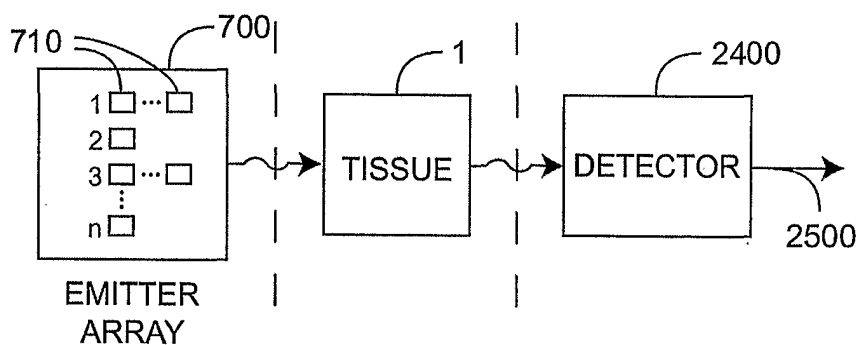


FIG. 10C

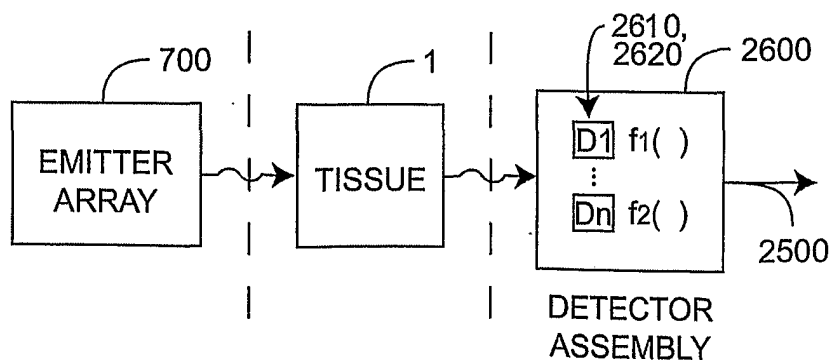


FIG. 10D

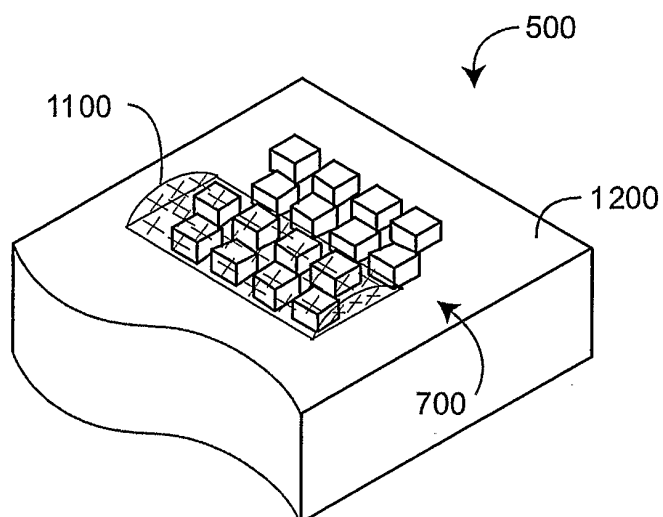


FIG. 11A

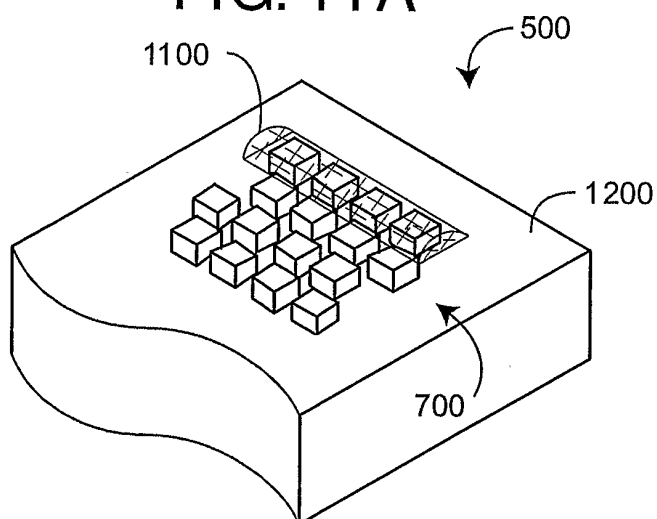


FIG. 11B

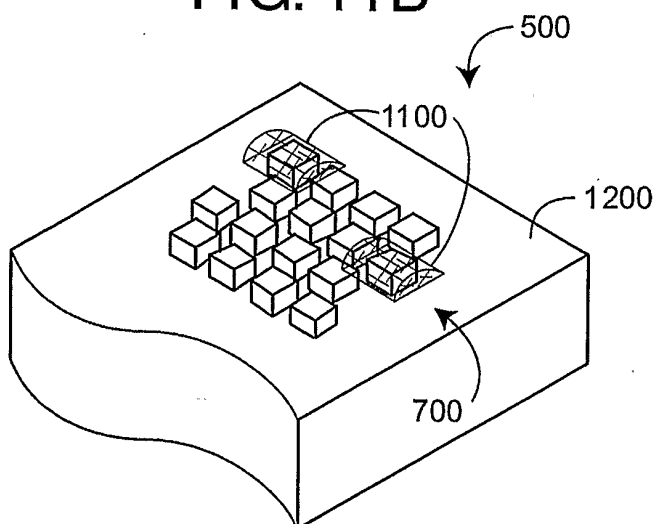


FIG. 11C

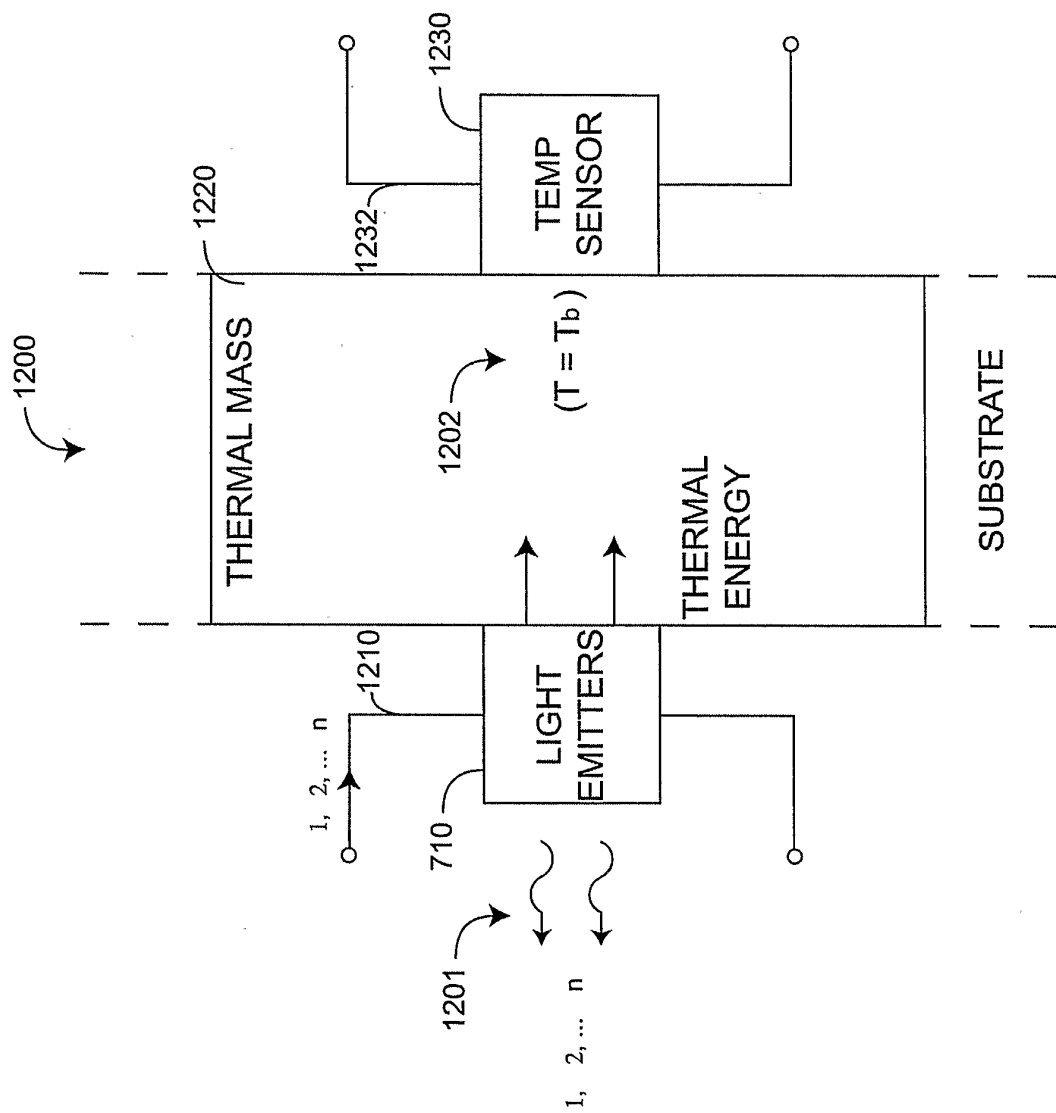
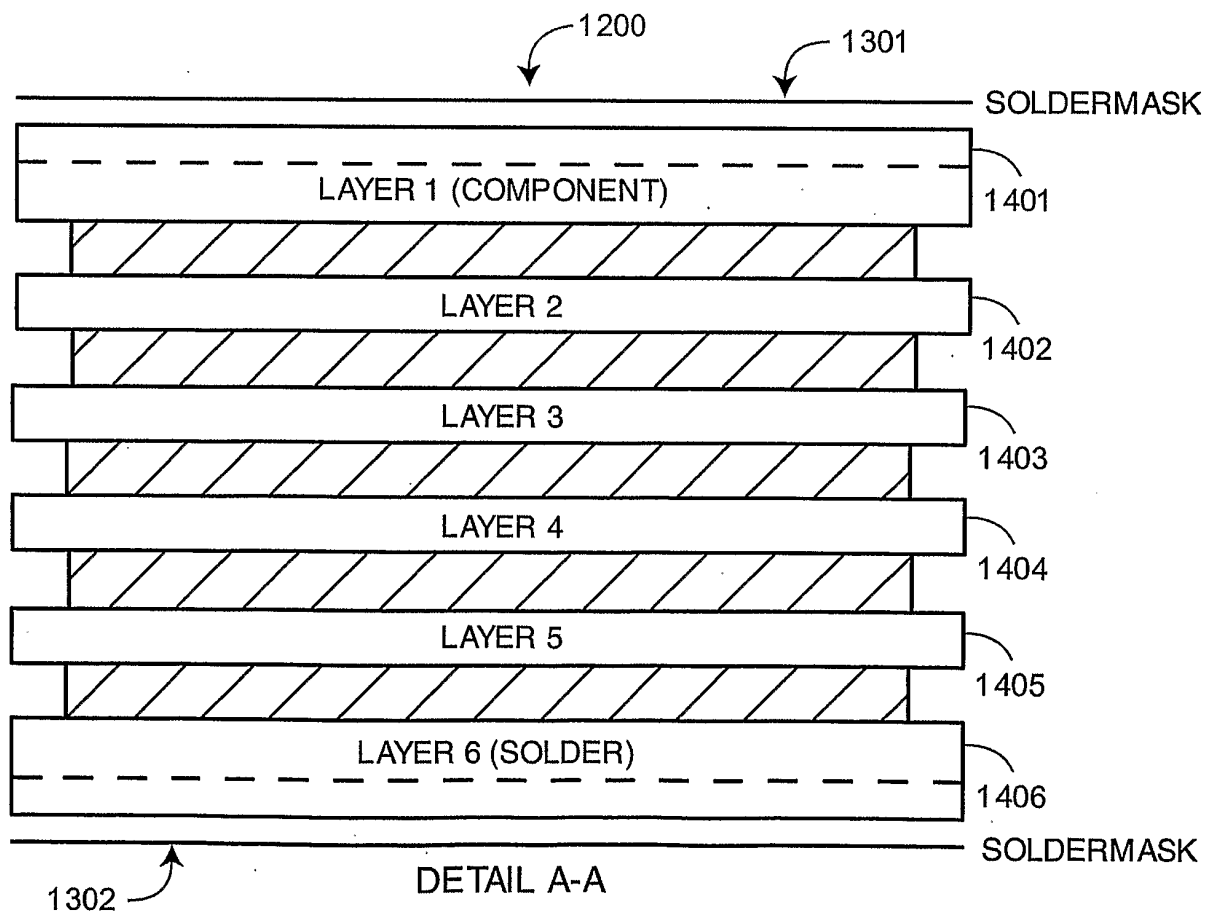
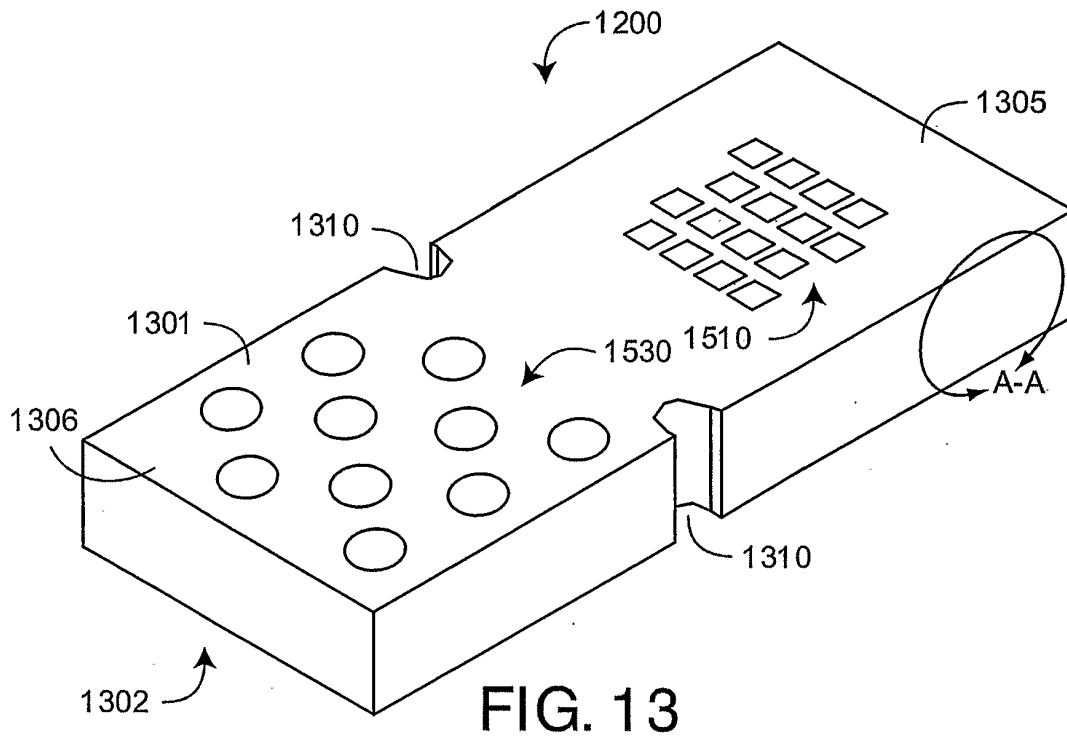


FIG. 12



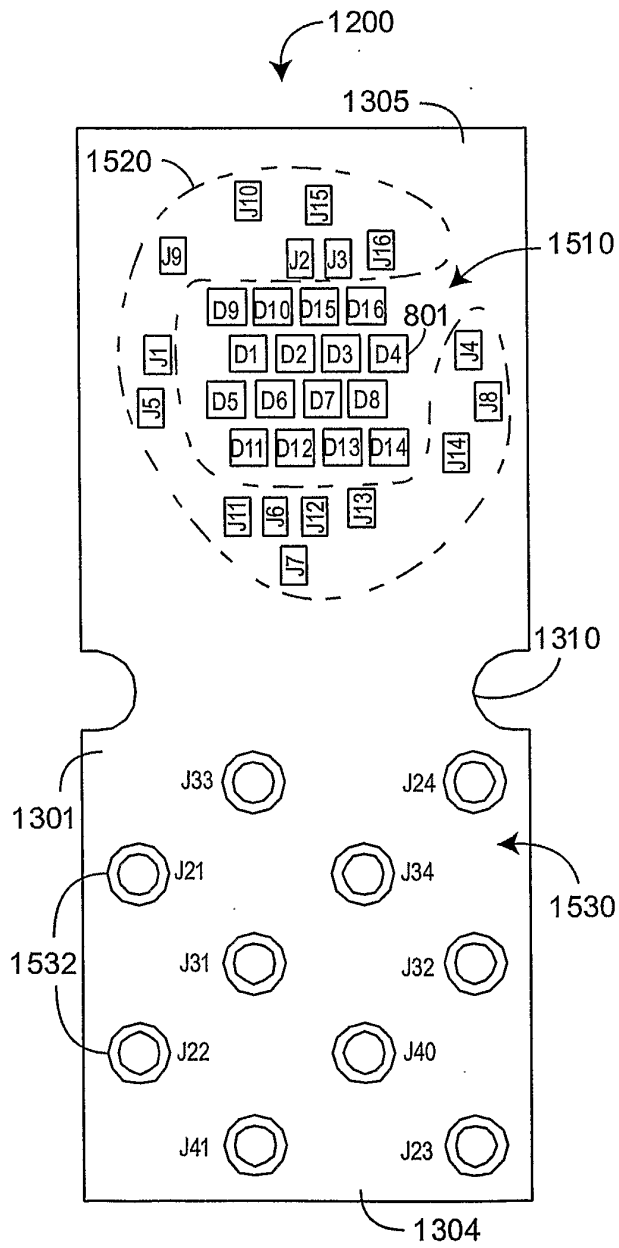


FIG. 15

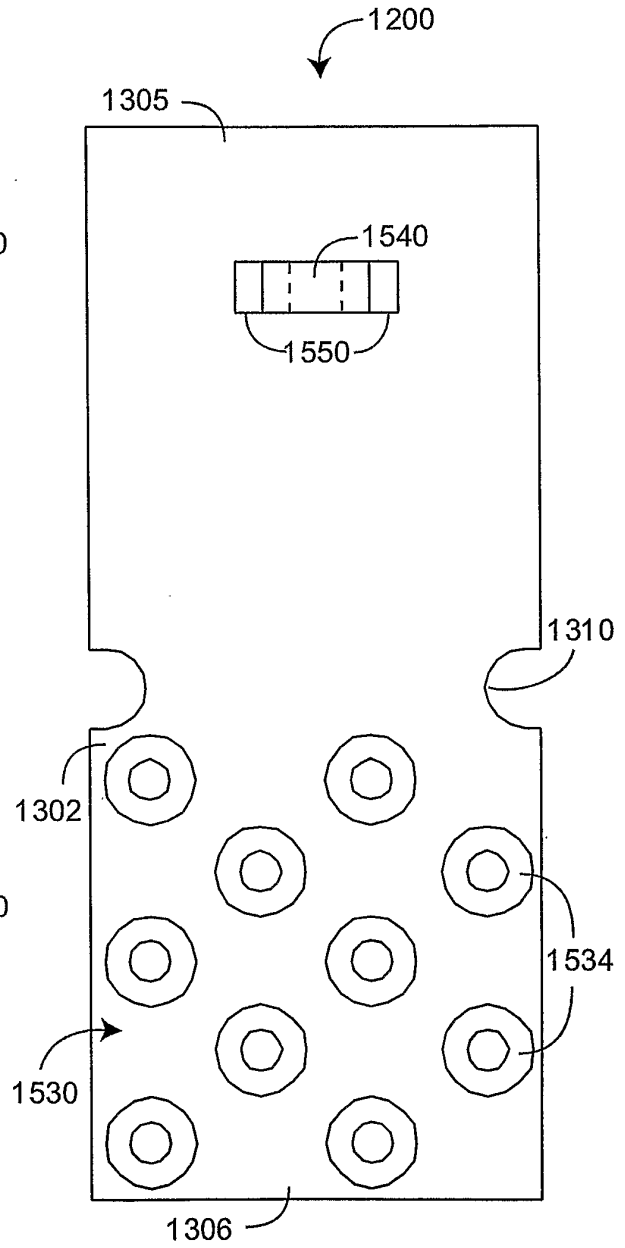


FIG. 16

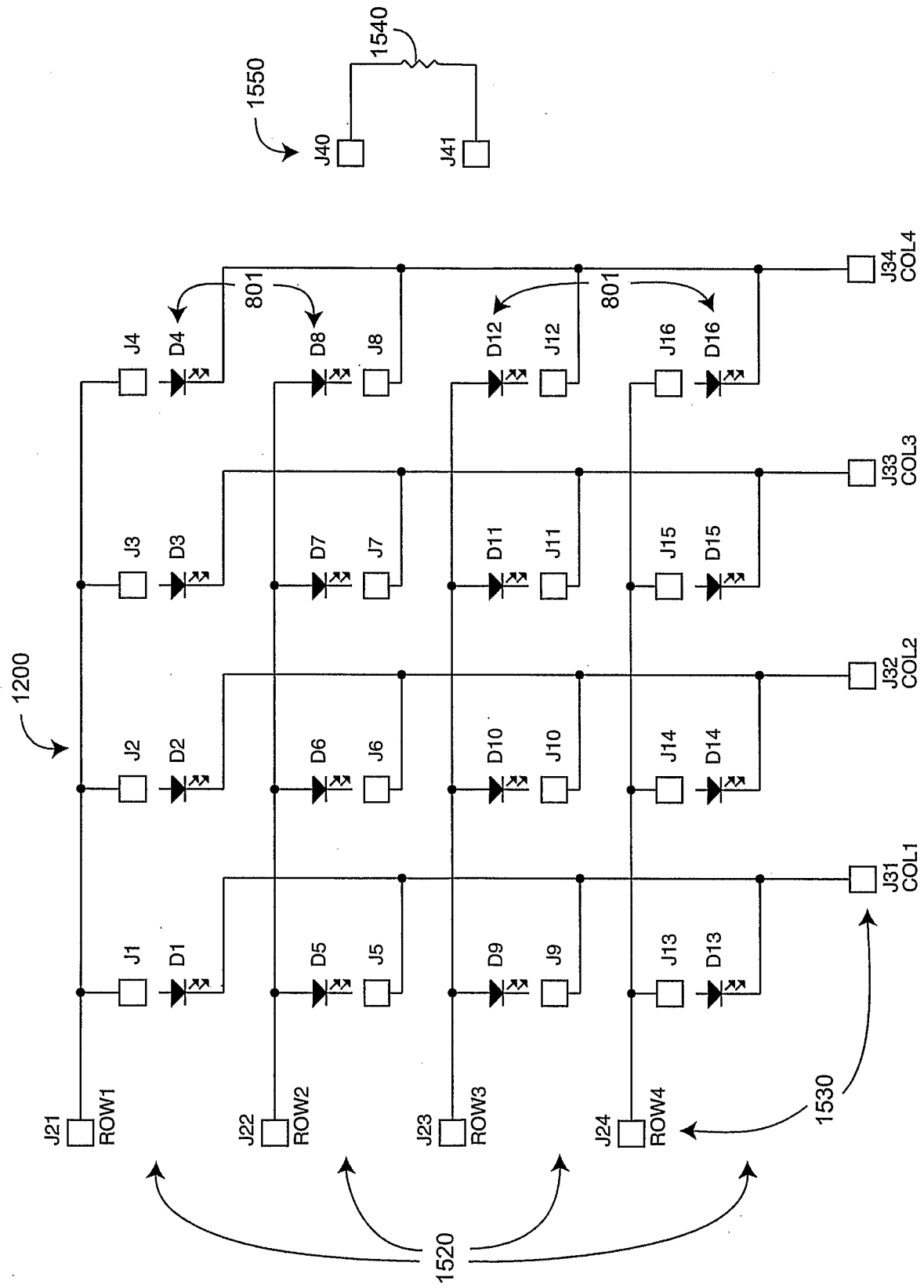


FIG. 17

1402

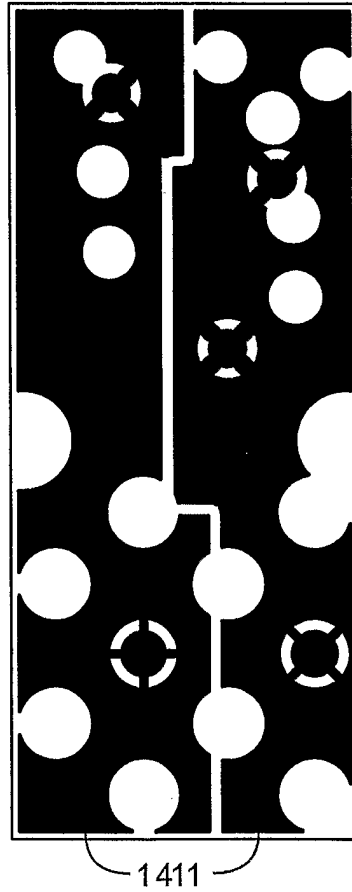


FIG. 18

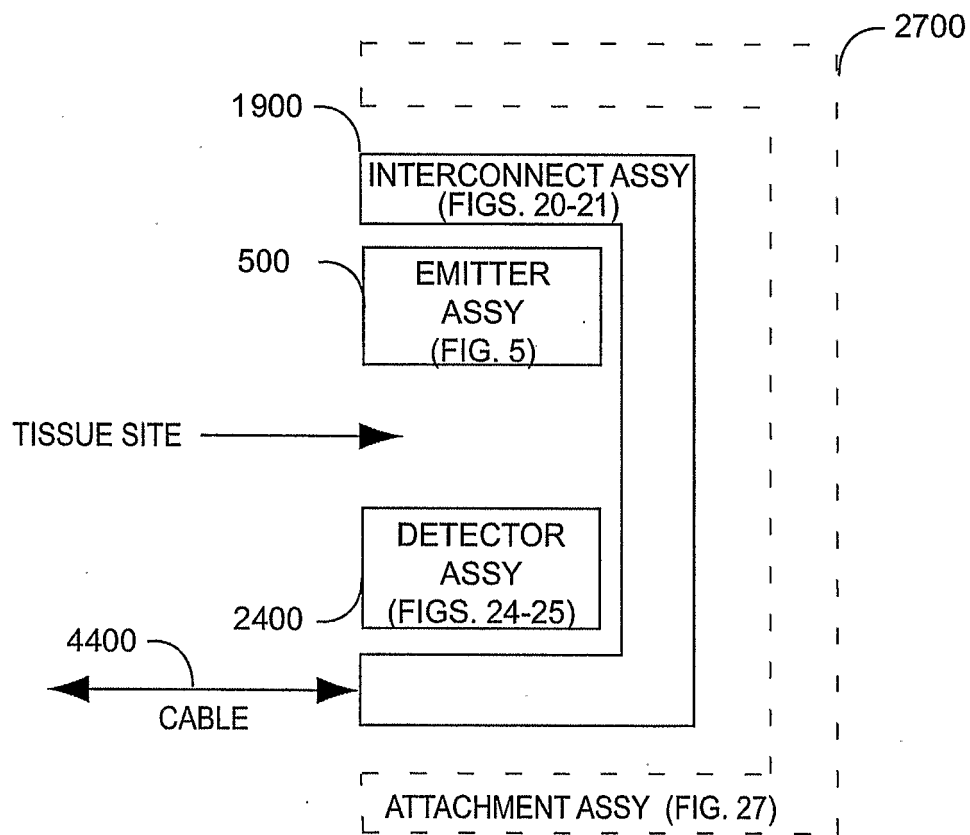


FIG. 19

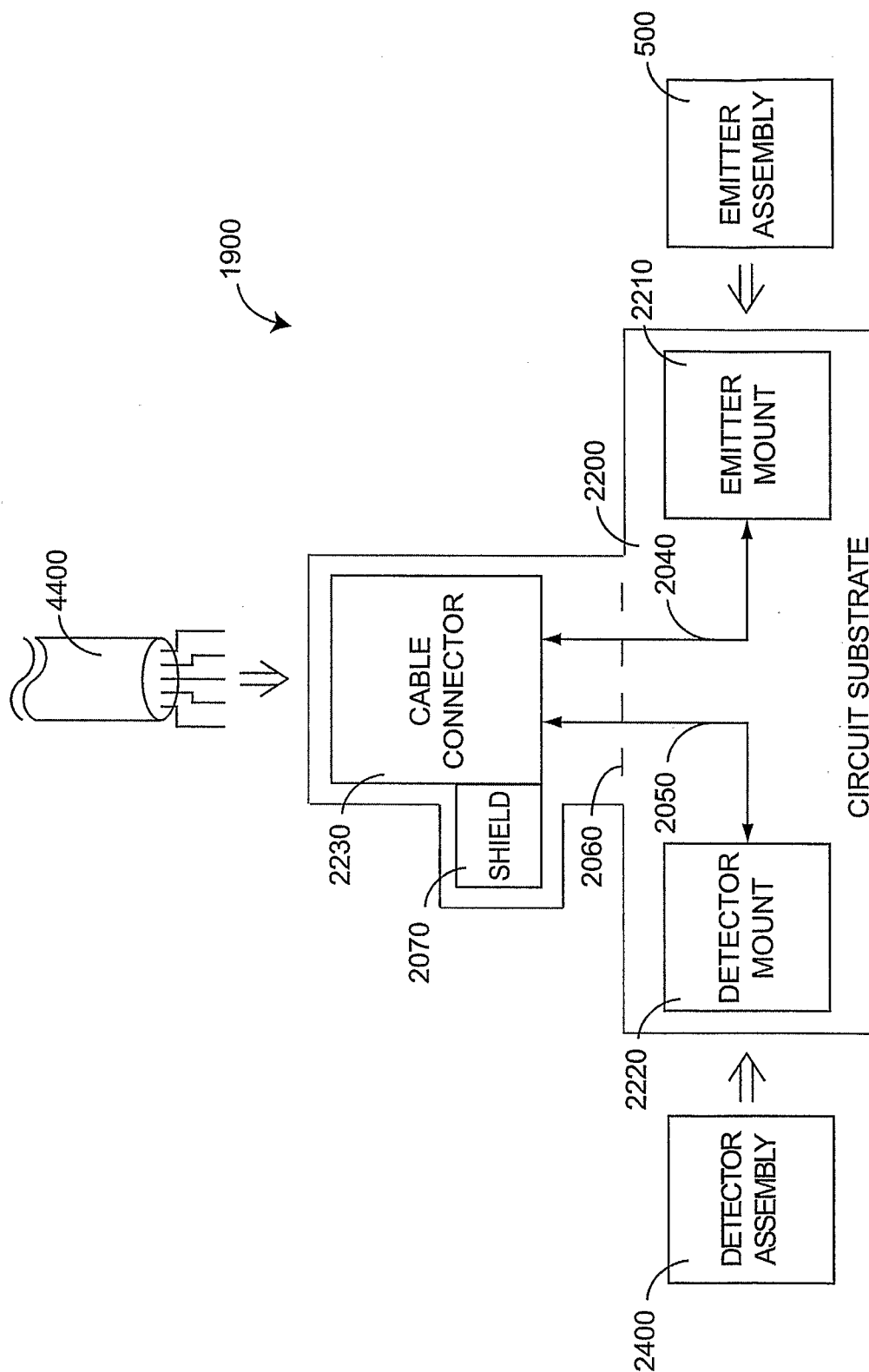


FIG. 20

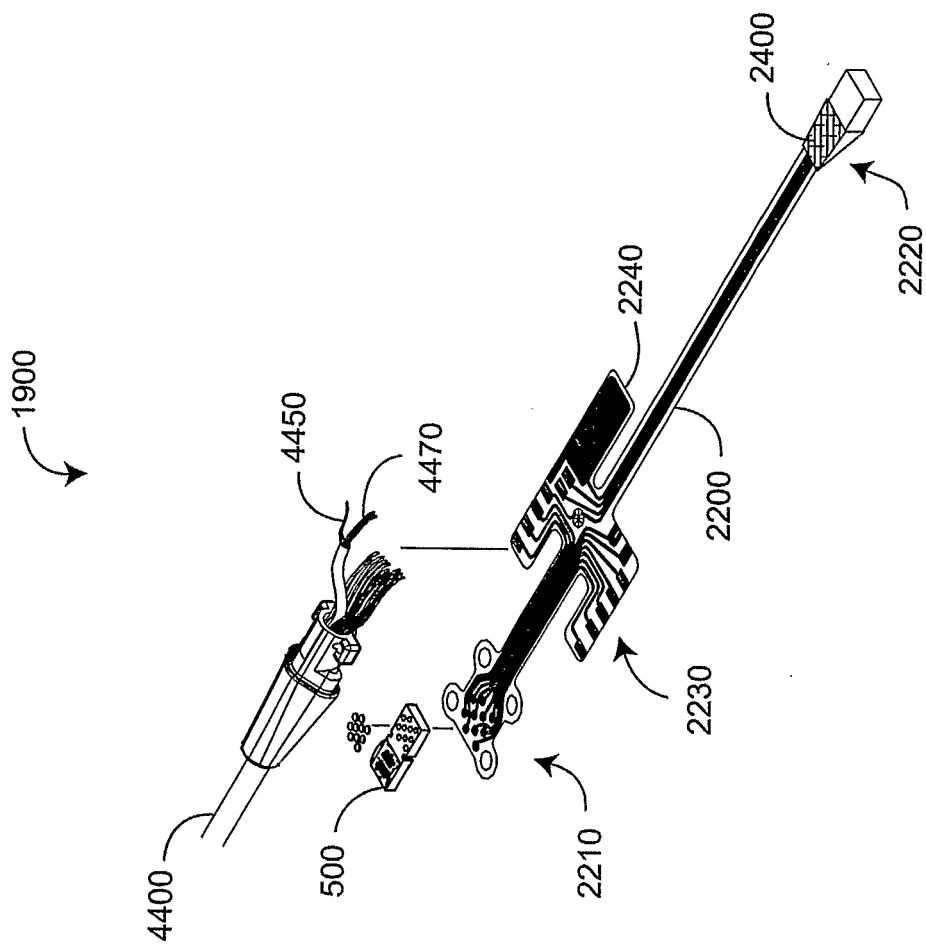


FIG. 21

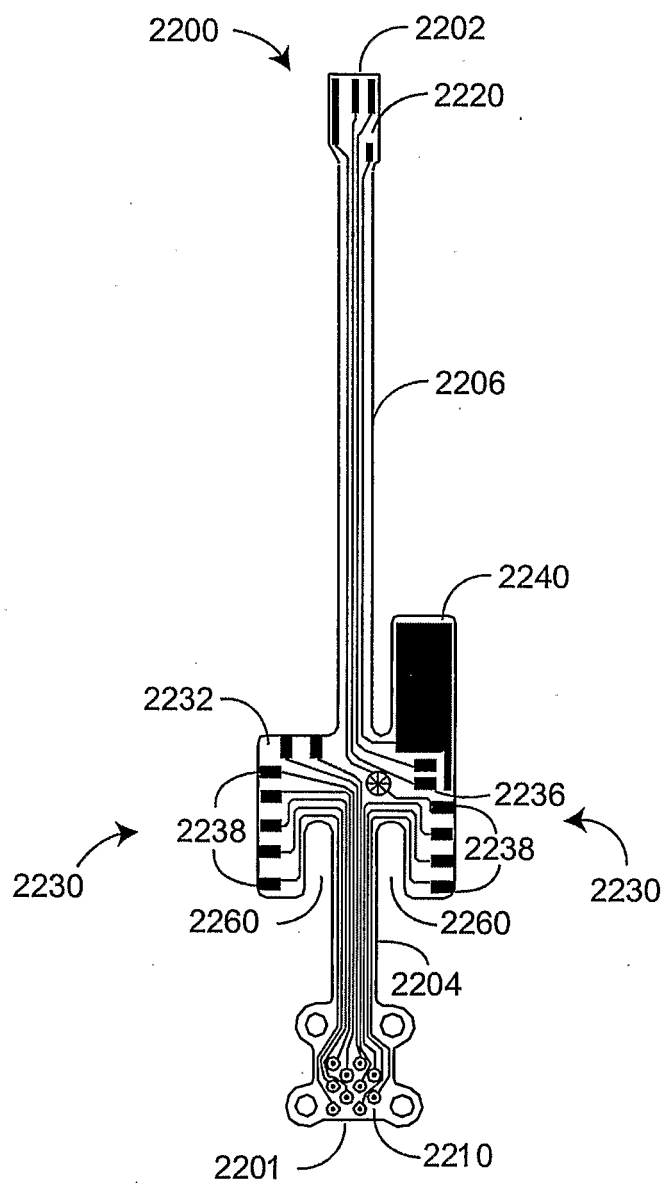


FIG. 22

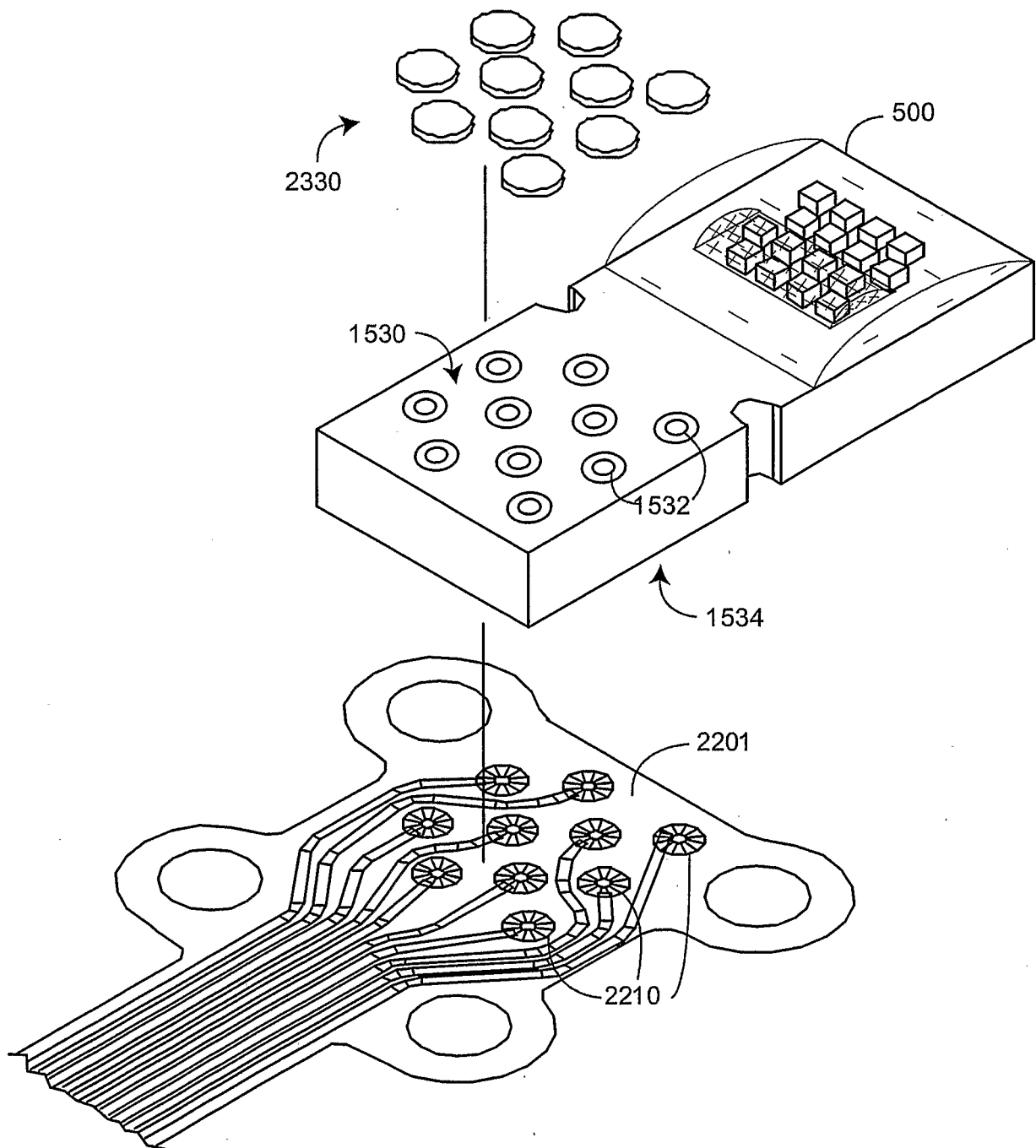


FIG. 23

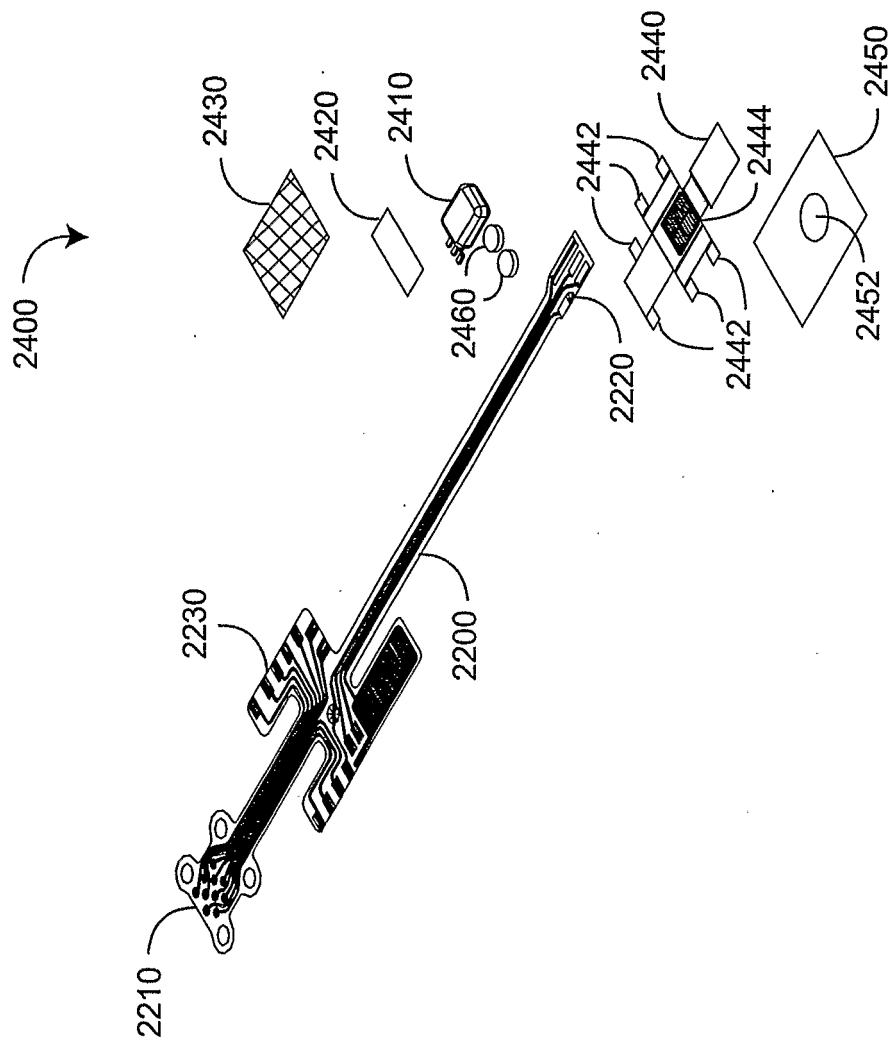


FIG. 24

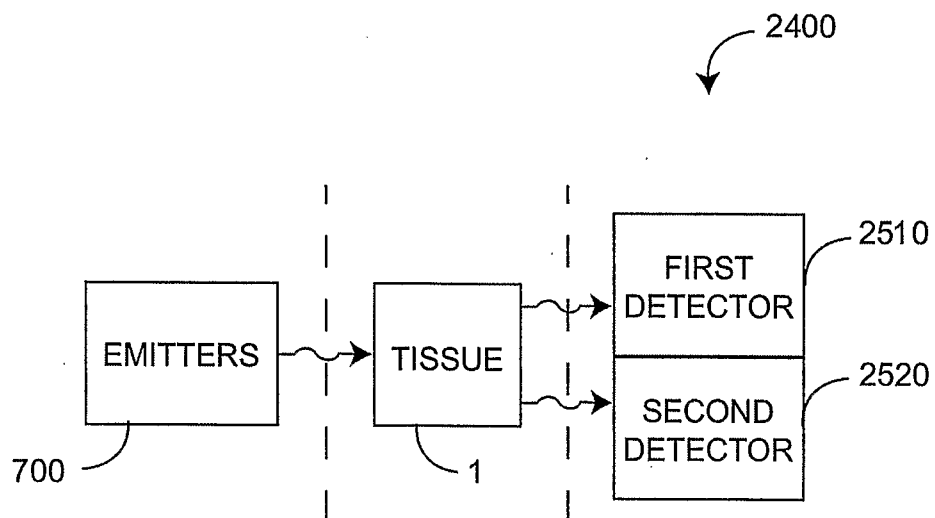


FIG. 25

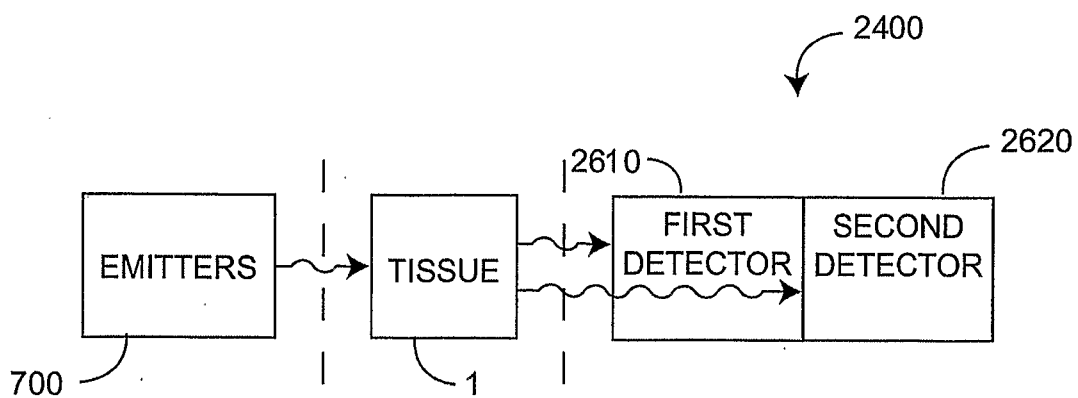


FIG. 26

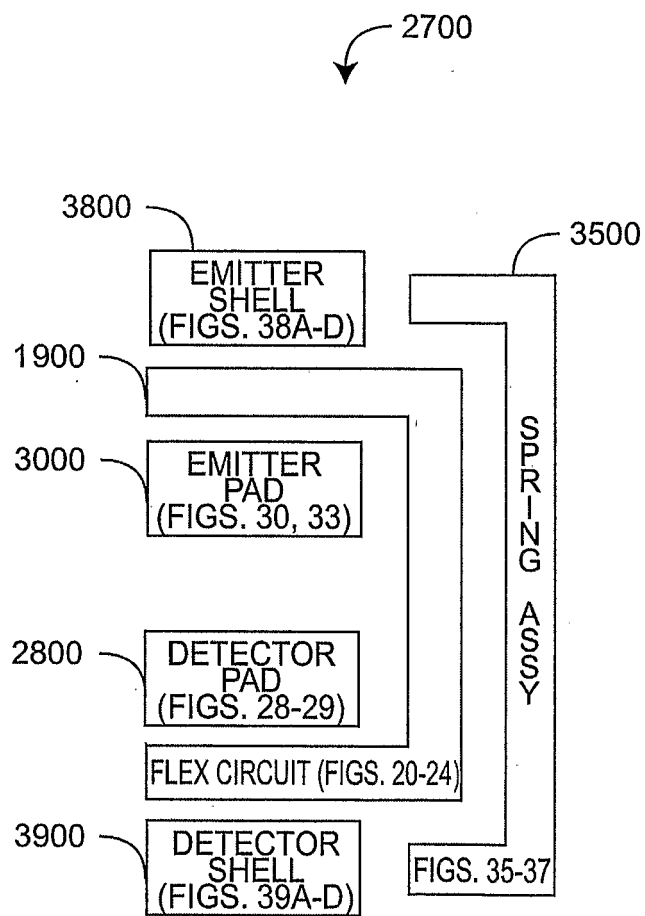


FIG. 27

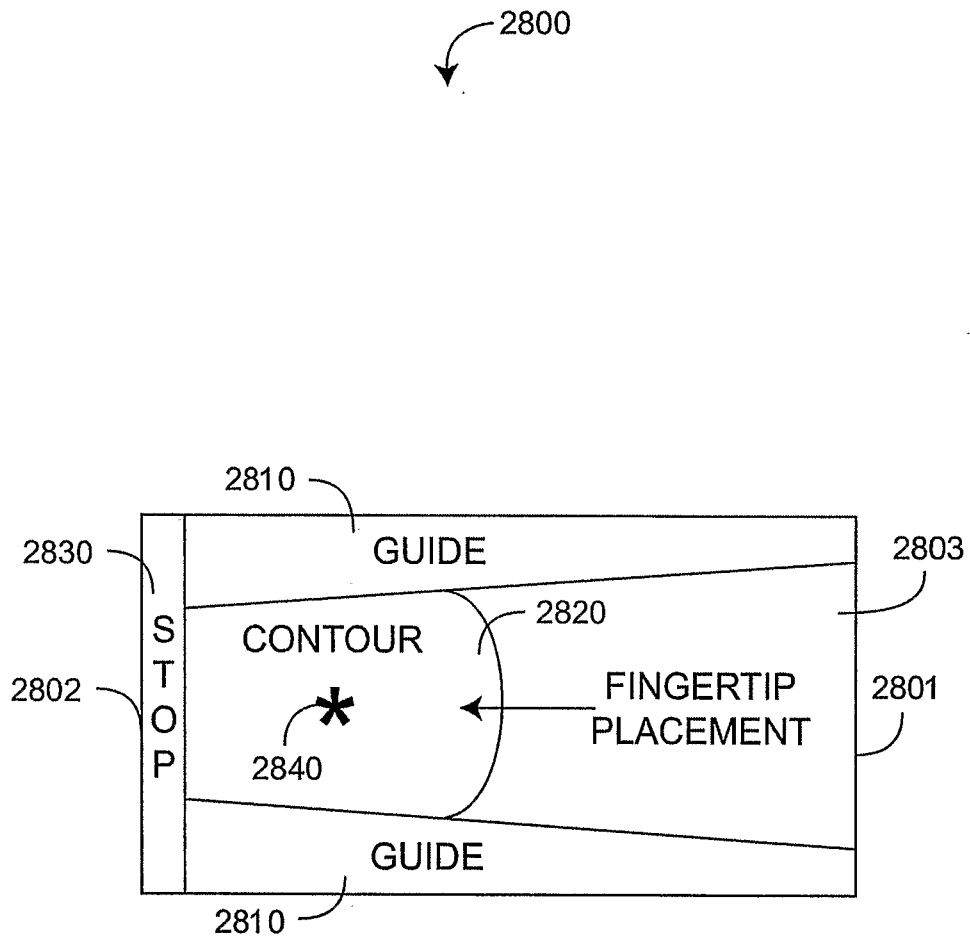


FIG. 28

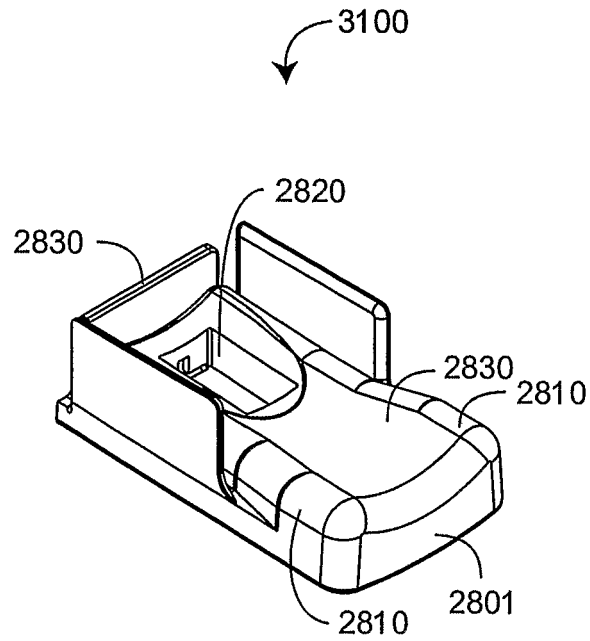


FIG. 29A

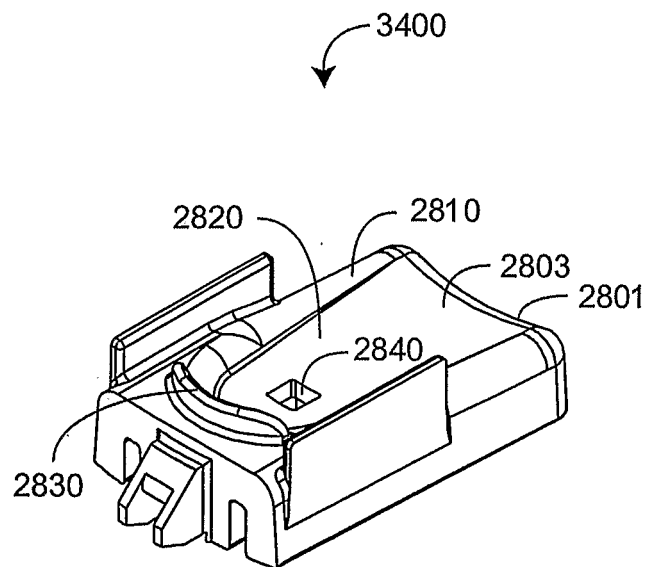


FIG. 29B

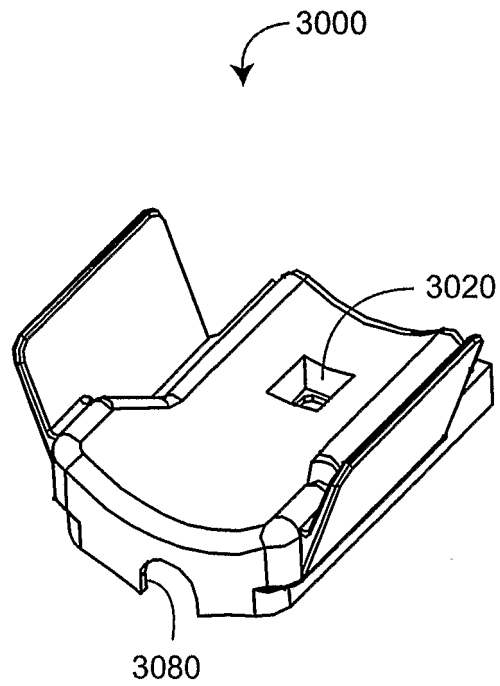


FIG. 30A

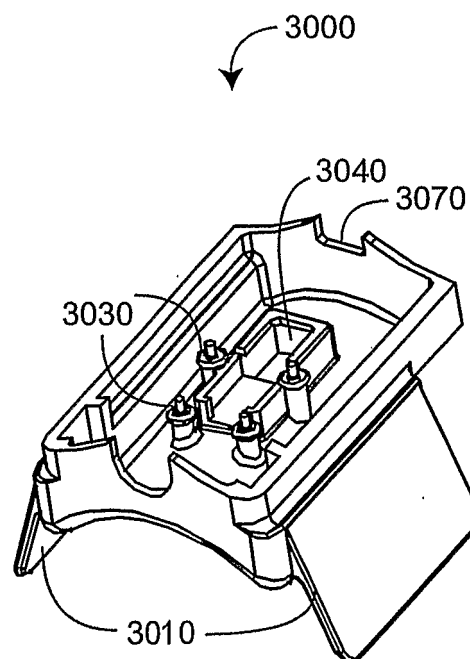


FIG. 30B

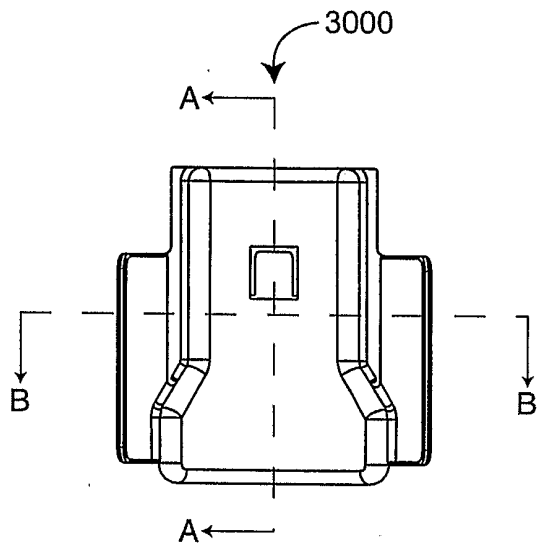
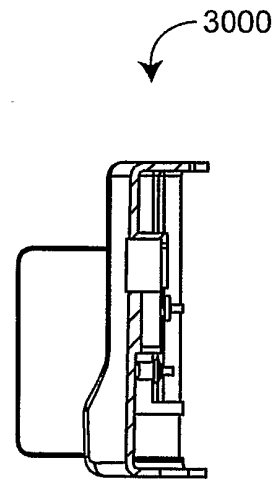


FIG. 30C



SECTION A-A

FIG. 30F

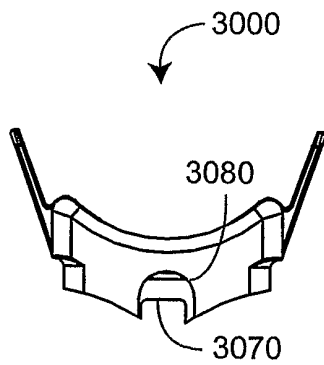


FIG. 30D

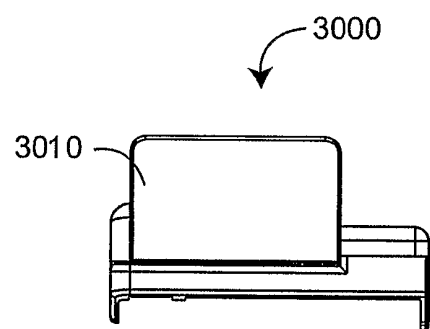


FIG. 30G

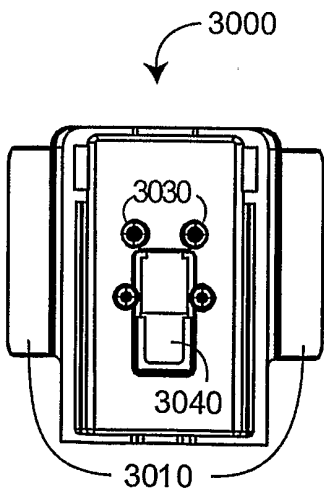
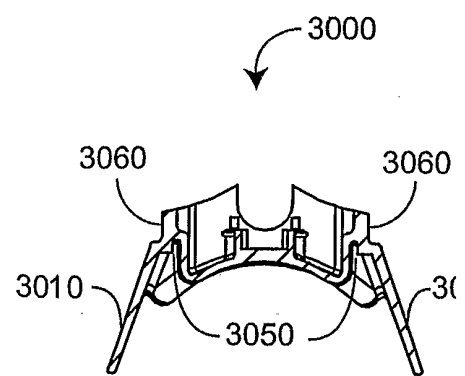


FIG. 30E



SECTION B-B

FIG. 30H

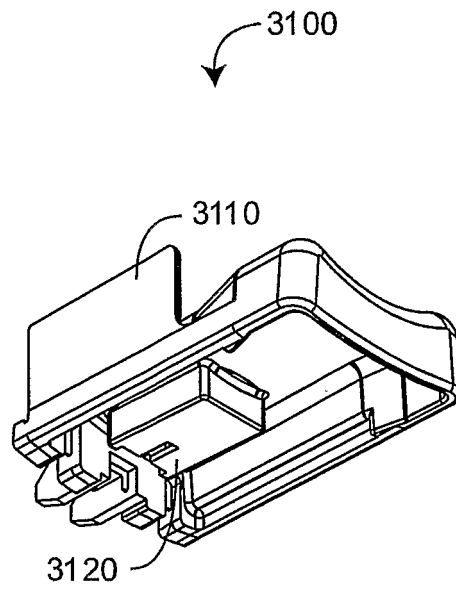


FIG. 31A

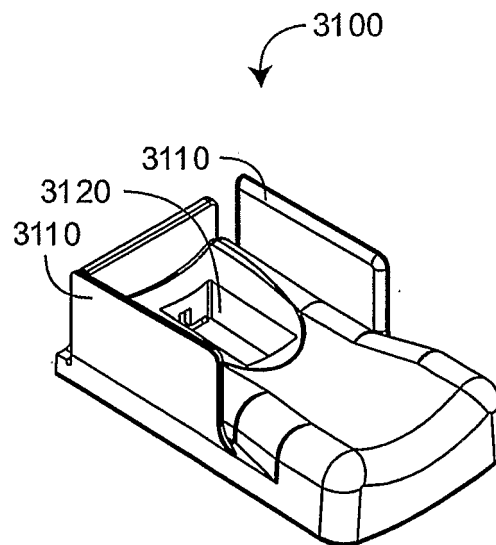


FIG. 31B

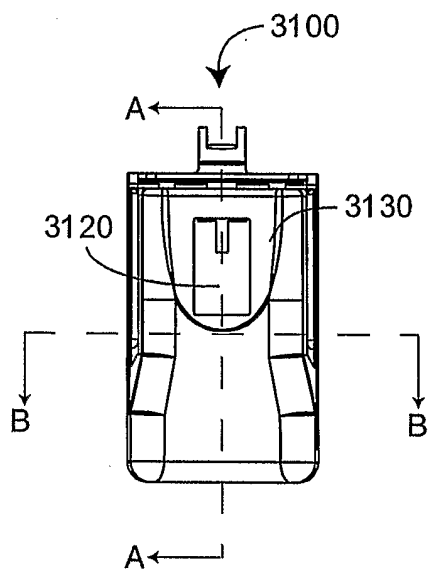
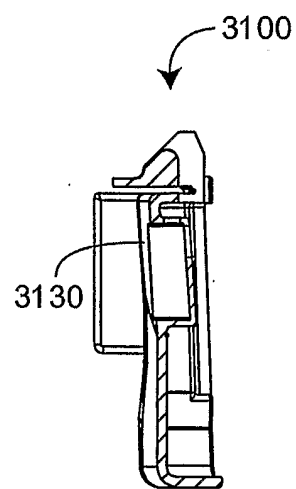


FIG. 31C



SECTION A-A

FIG. 31F

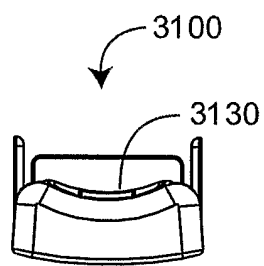


FIG. 31D

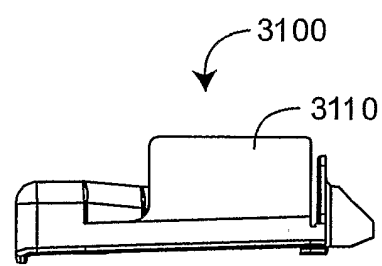


FIG. 31G

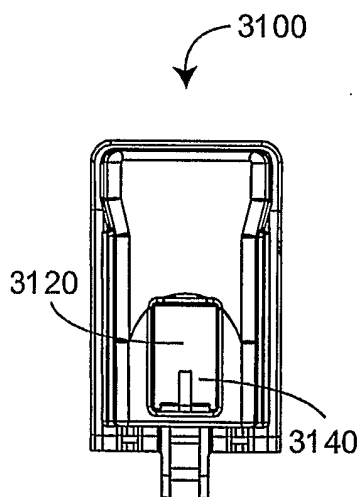
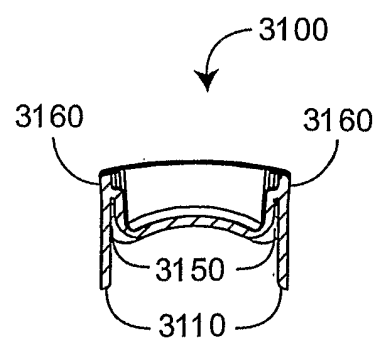


FIG. 31E



SECTION B-B

FIG. 31H

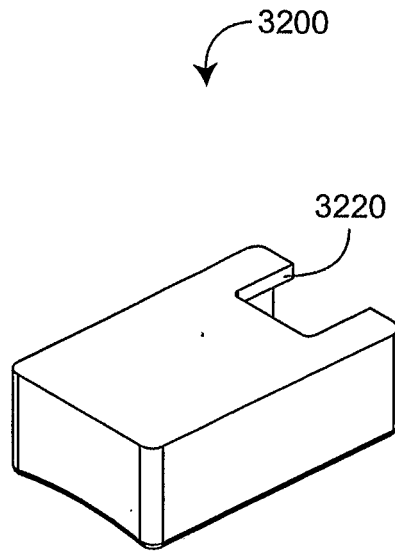


FIG. 32A

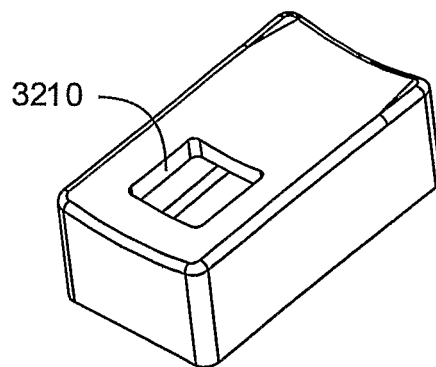


FIG. 32B

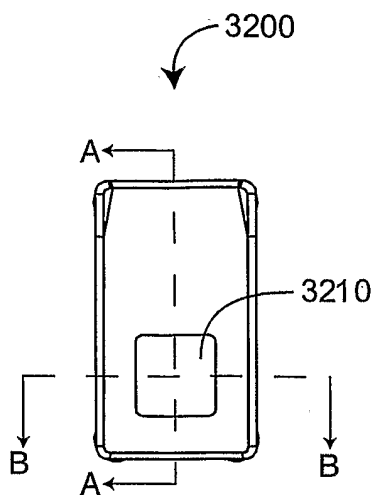


FIG. 32C

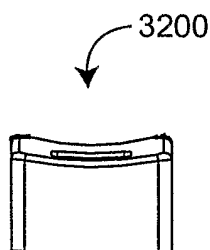


FIG. 32D

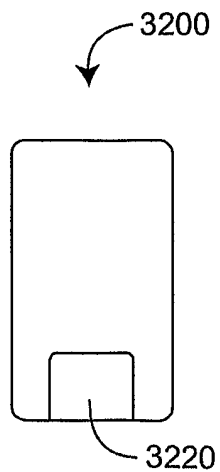
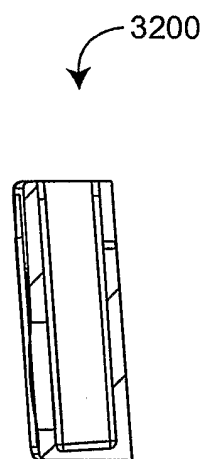


FIG. 32E



SECTION A-A

FIG. 32F

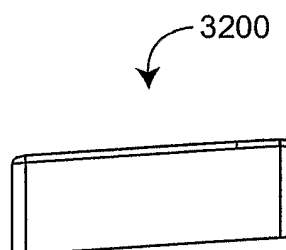
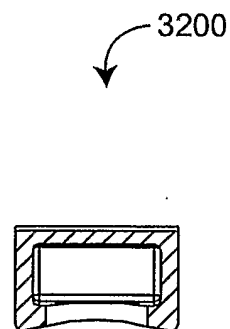


FIG. 32G



SECTION B-B

FIG. 32H

3300

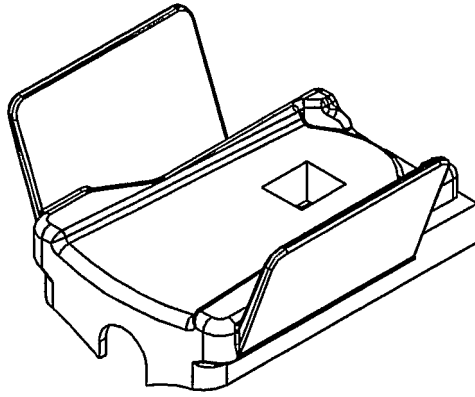


FIG. 33A

3300

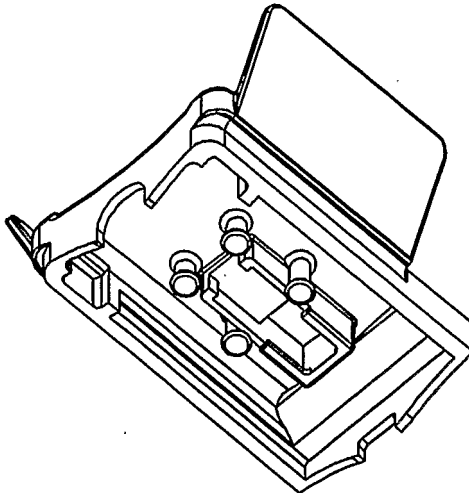


FIG. 33B

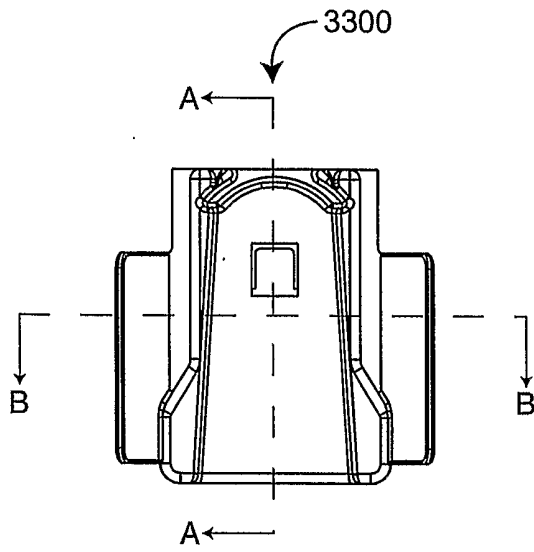
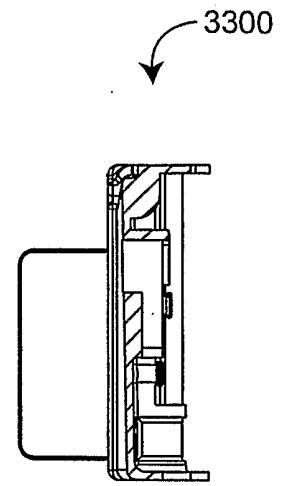


FIG. 33C



SECTION A-A

FIG. 33F

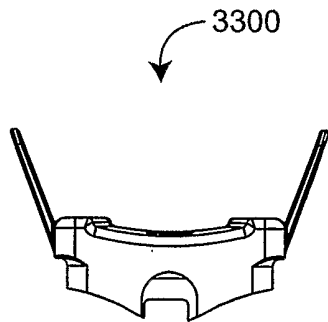


FIG. 33D

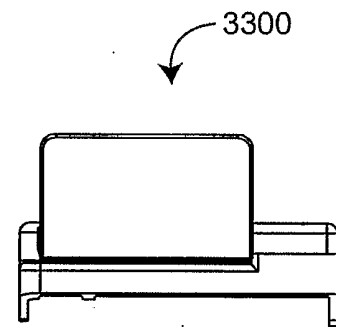


FIG. 33G

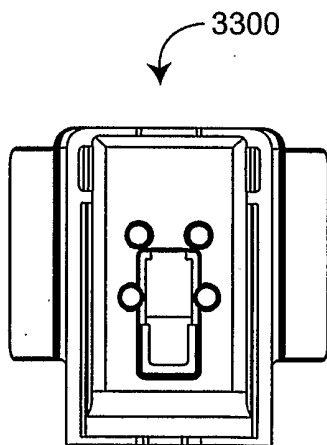
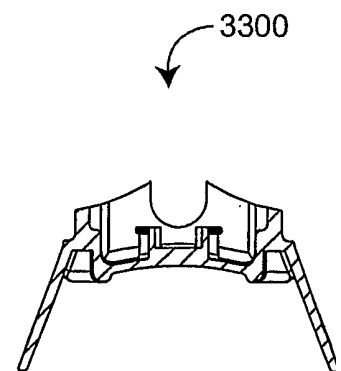


FIG. 33E



SECTION B-B

FIG. 33H

3400

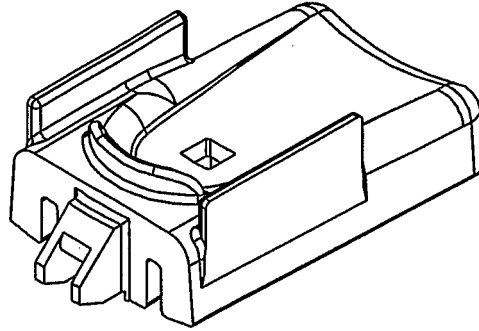


FIG. 34A

3400

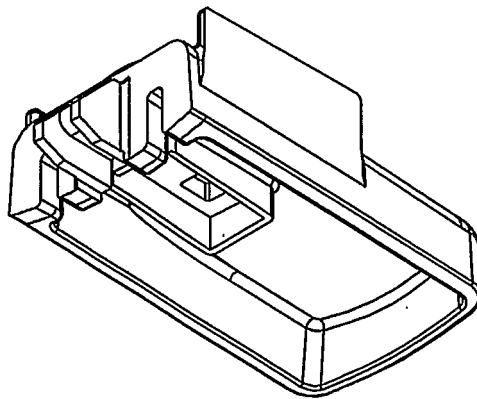


FIG. 34B

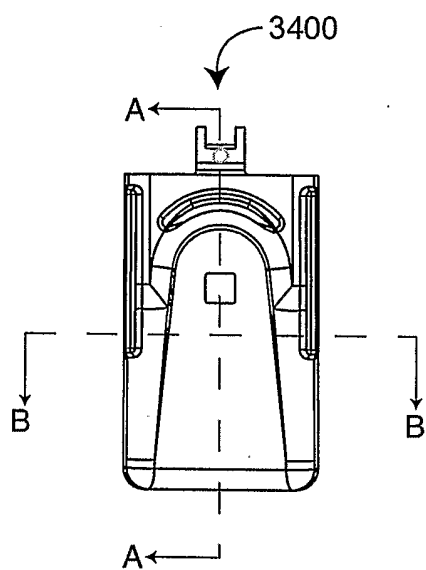
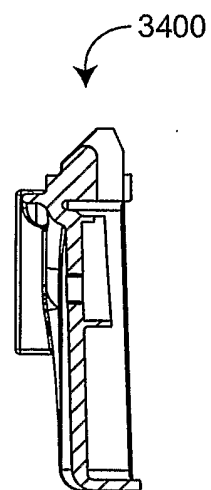


FIG. 34C



SECTION A-A

FIG. 34F

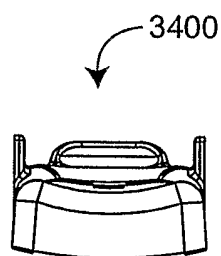


FIG. 34D

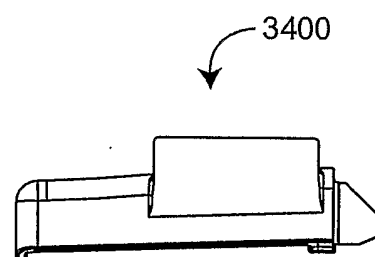


FIG. 34G

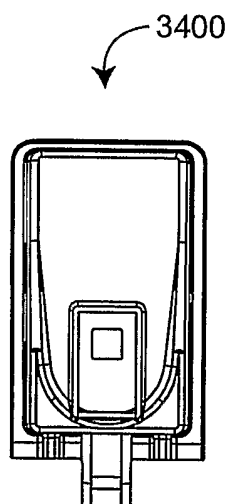
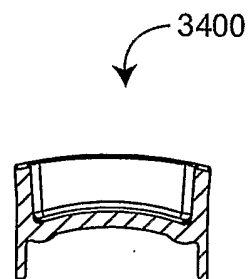


FIG. 34E



SECTION B-B

FIG. 34H

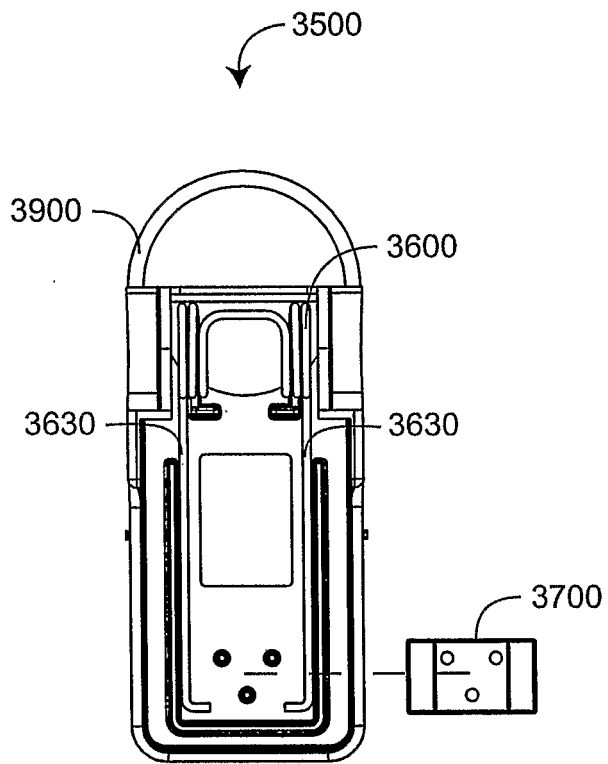


FIG. 35A

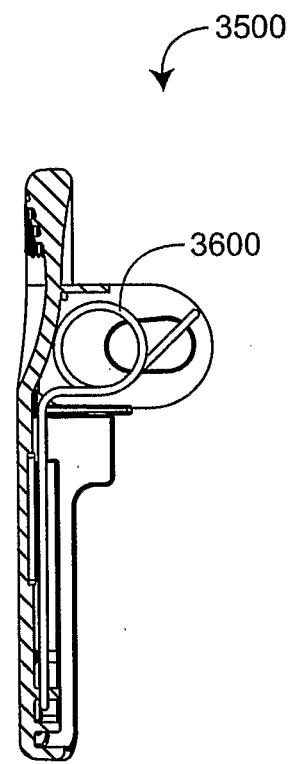


FIG. 35B

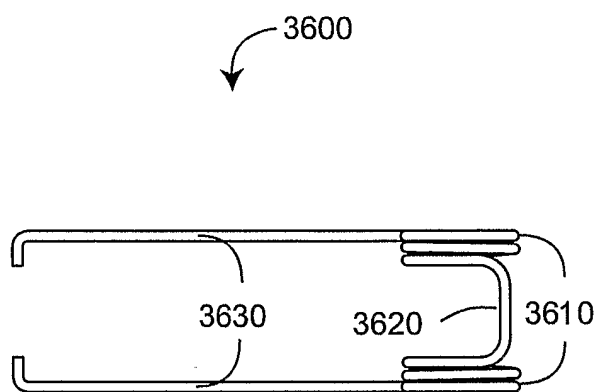


FIG. 36A

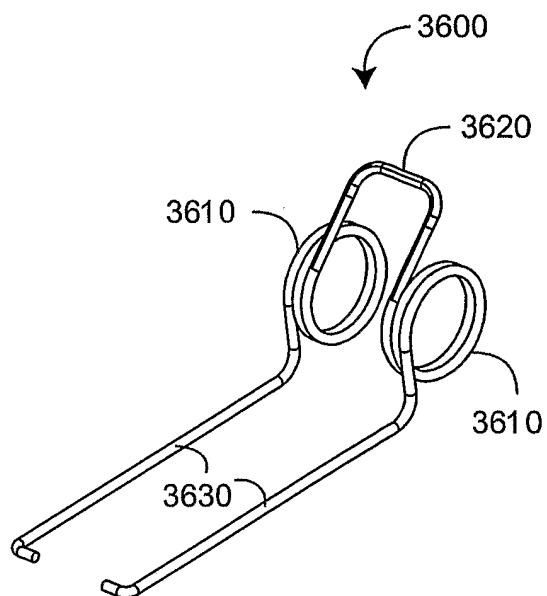


FIG. 36B

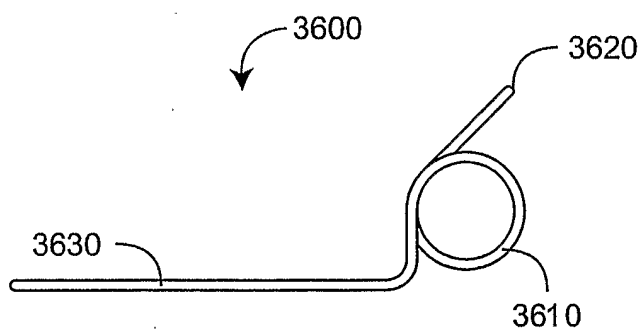


FIG. 36C

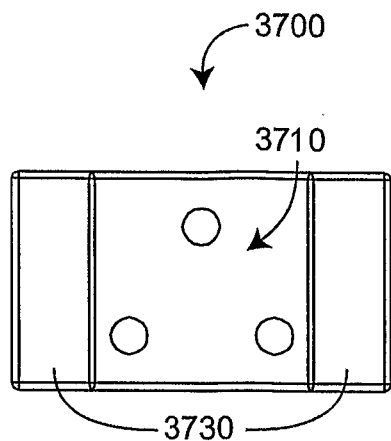


FIG. 37A

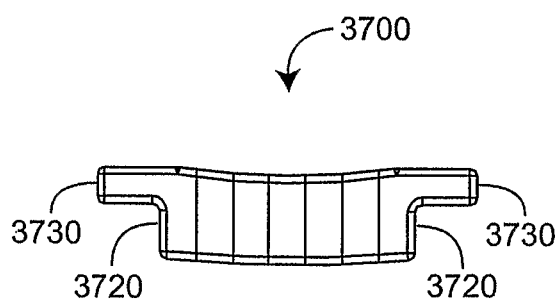


FIG. 37B

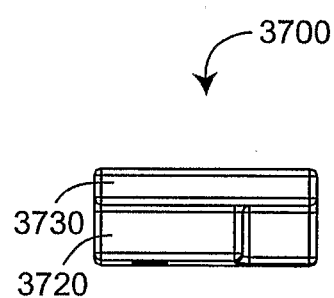


FIG. 37D

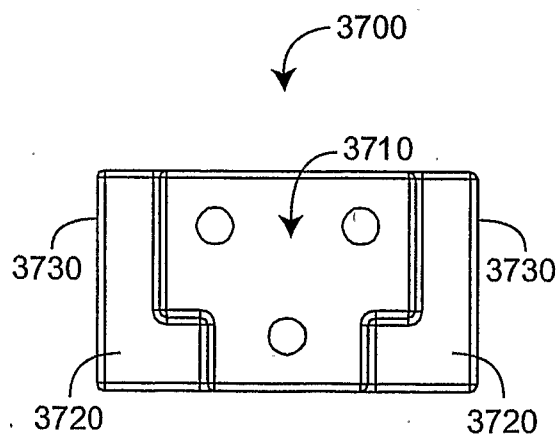


FIG. 37C

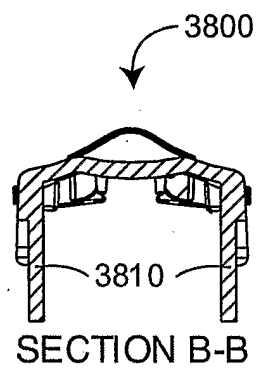


FIG. 38A

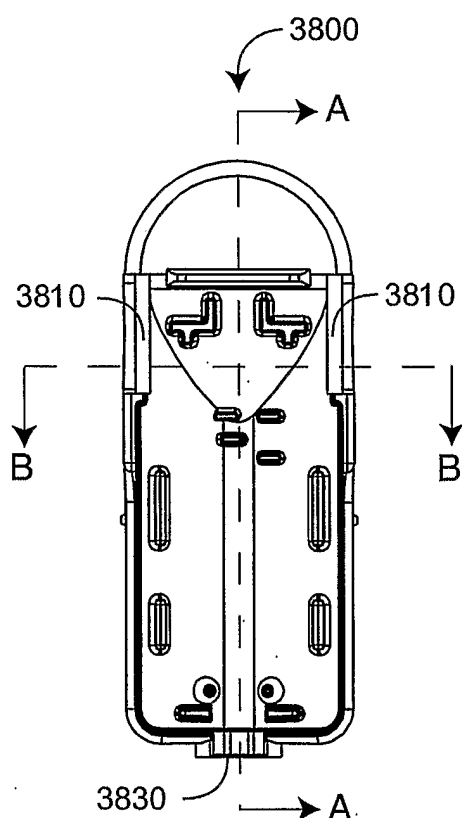


FIG. 38B

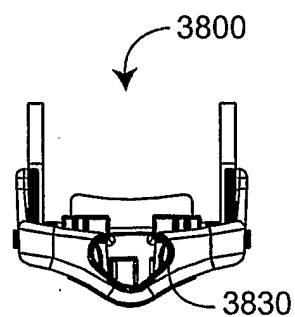
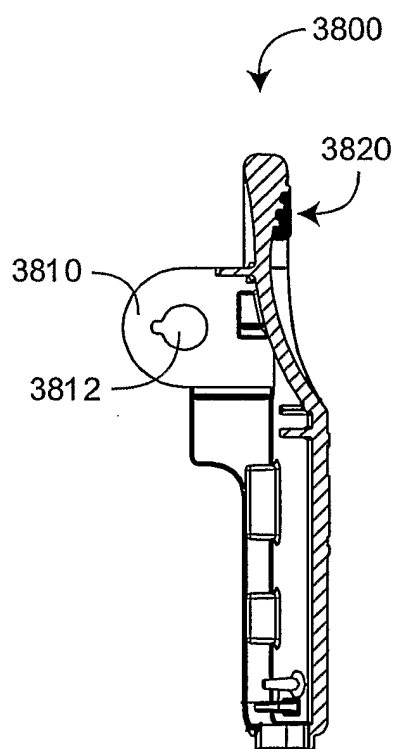


FIG. 38C



SECTION A-A  
FIG. 38D

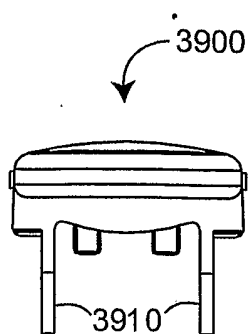


FIG. 39A

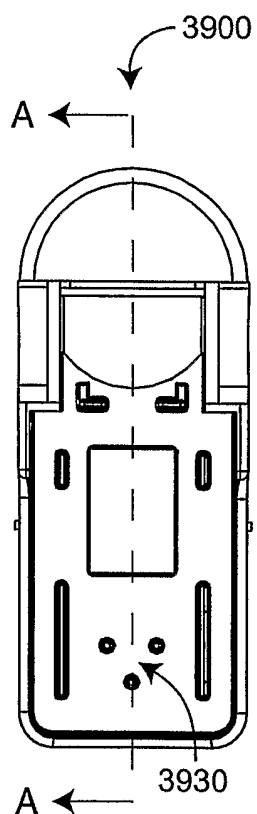
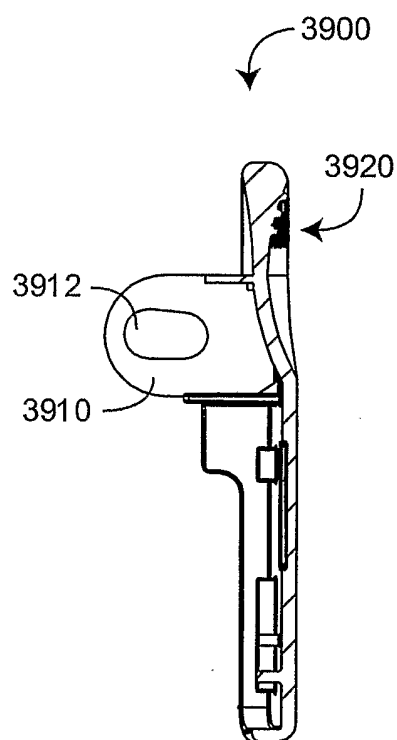


FIG. 39B



SECTION A-A  
FIG. 39D

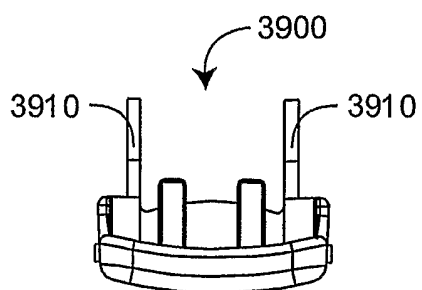


FIG. 39C

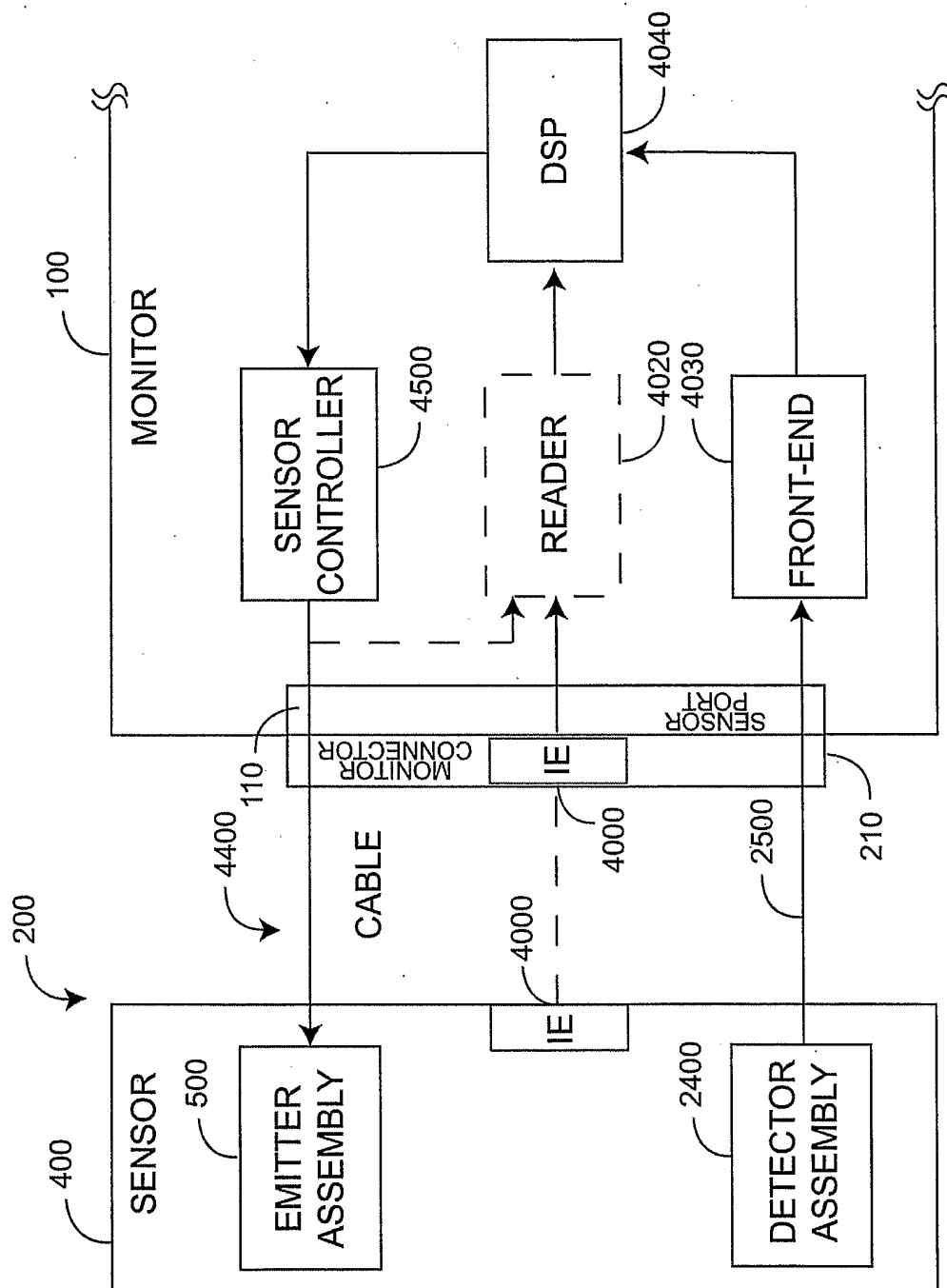


FIG. 40

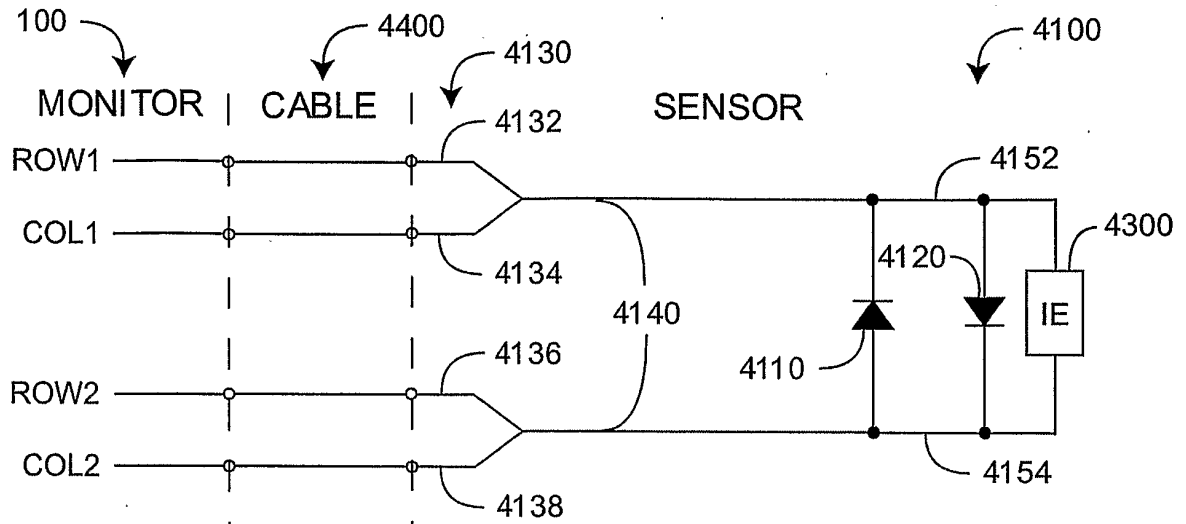


FIG. 41A

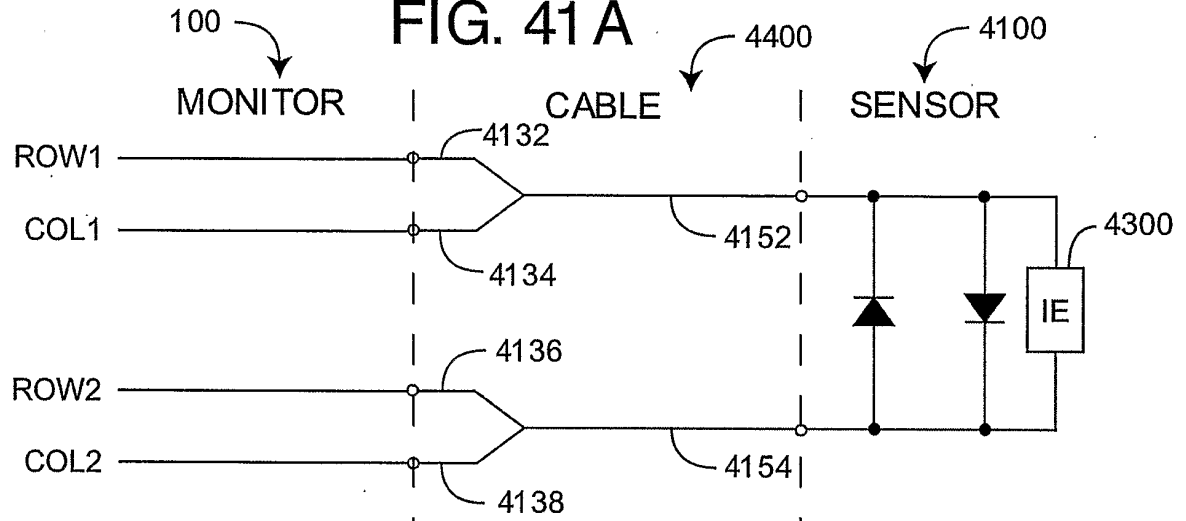


FIG. 41B

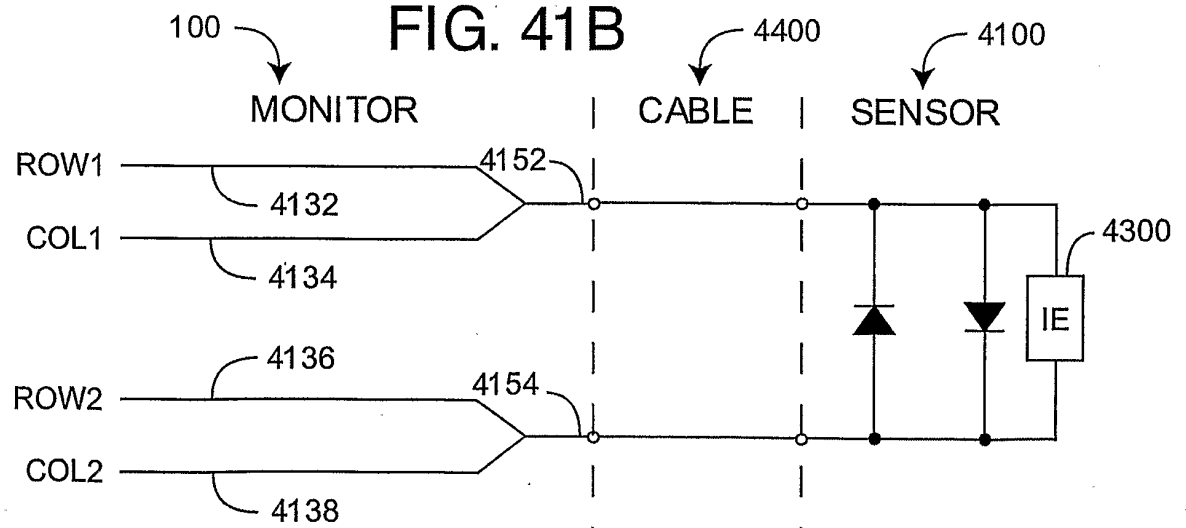
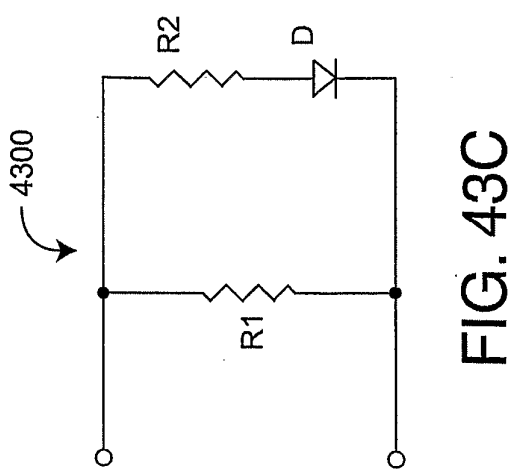
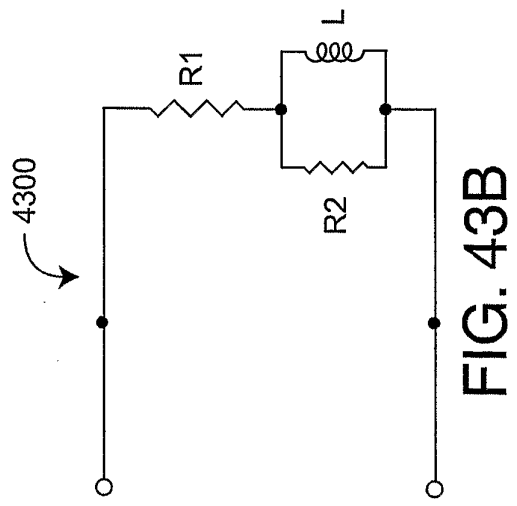
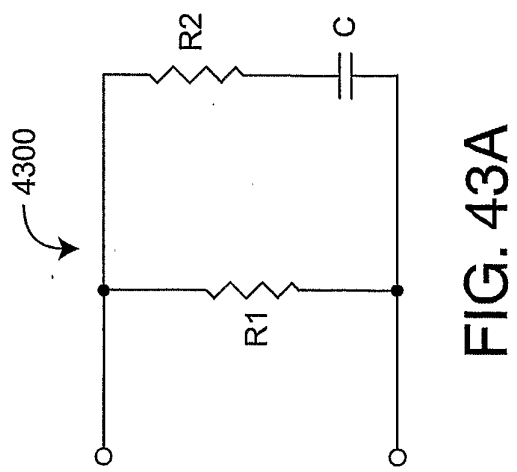
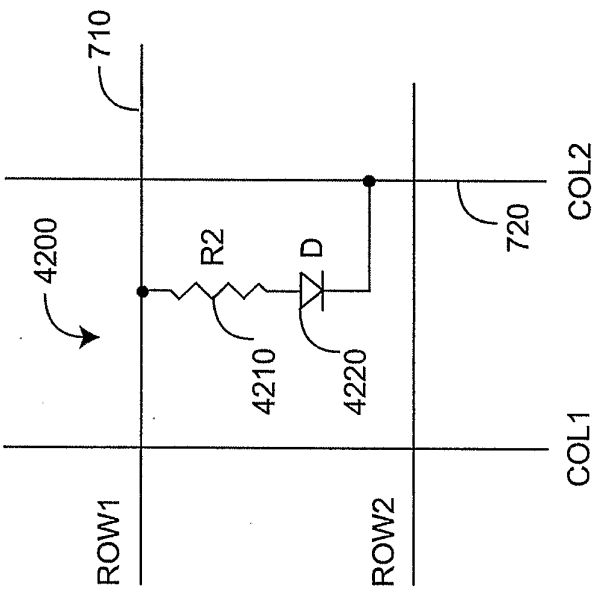


FIG. 41C



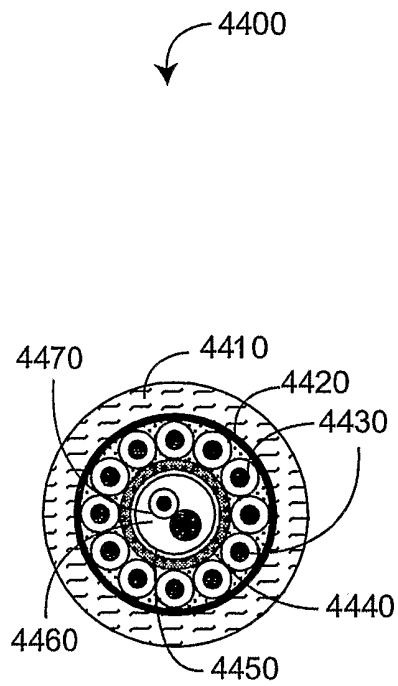


FIG. 44A

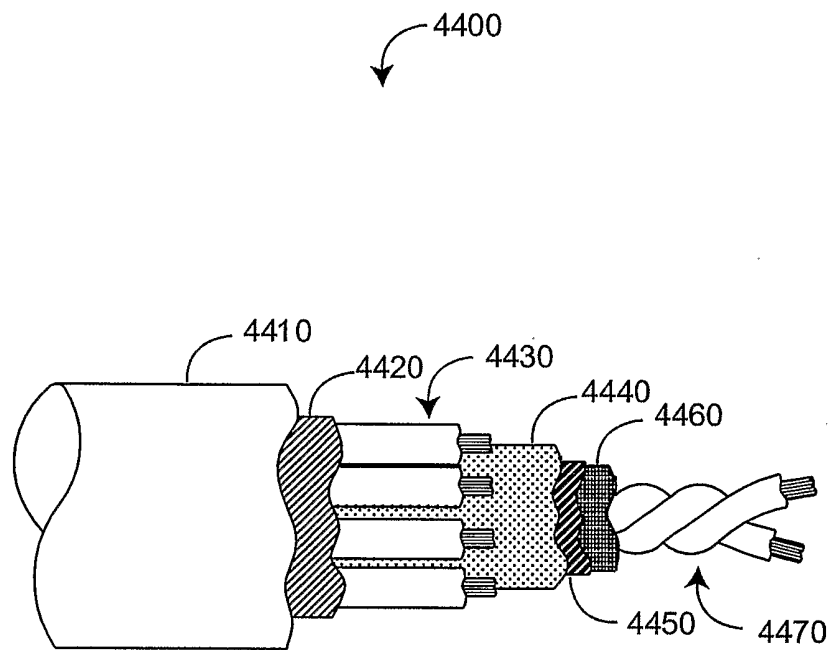


FIG. 44B

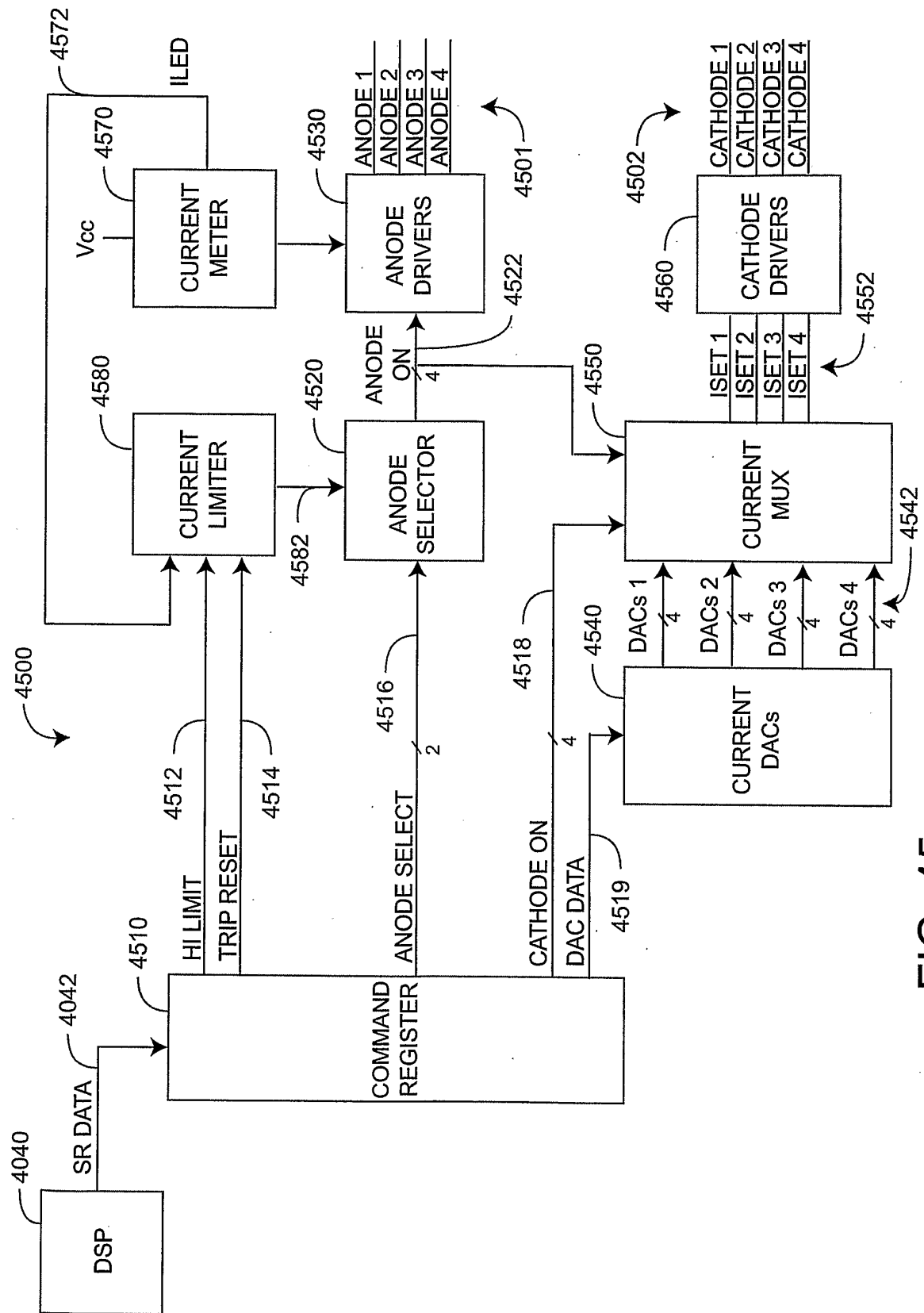


FIG. 45

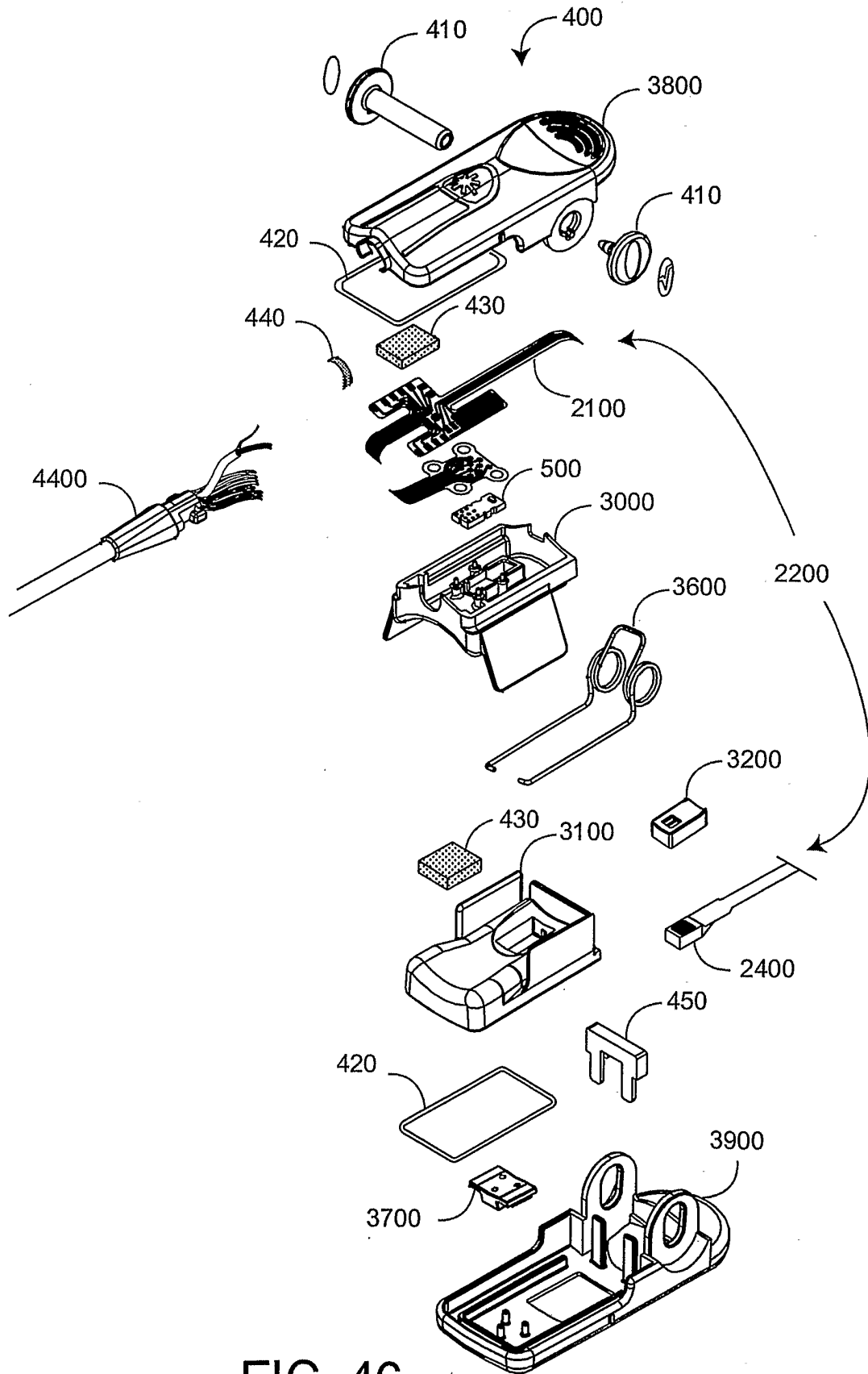


FIG. 46

**REFERENCES CITED IN THE DESCRIPTION**

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专利名称(译)	多波长传感器发射器		
公开(公告)号	<a href="#">EP1860994B1</a>	公开(公告)日	2019-10-16
申请号	EP2006736798	申请日	2006-03-01
[标]申请(专利权)人(译)	MASIMO LAB		
申请(专利权)人(译)	MASIMO实验室, INC.		
当前申请(专利权)人(译)	MASIMO实验室, INC.		
[标]发明人	AL ALI AMMAR DIAB MOHAMED LAMEGO MARCELO SMITH ROBERT DALKE DAVID		
发明人	AL-ALI, AMMAR DIAB, MOHAMED LAMEGO, MARCELO SMITH, ROBERT DALKE, DAVID		
IPC分类号	A61B5/00		
CPC分类号	A61B5/02416 A61B5/14552 A61B5/6832 A61B5/746 A61B2562/08 A61B2562/085 A61B2562/222 G06F19/3418 G16H10/40 G16H40/67 Y10S439/909 A61B1/00 A61B5/0022 A61B5/0205 A61B5/02427 A61B5/0261 A61B5/0295 A61B5/14532 A61B5/14546 A61B5/1455 A61B5/14551 A61B5/1495 A61B5/ /6815 A61B5/6826 A61B5/6829 A61B5/6838 A61B5/7221 A61B5/7246 A61B5/7275 A61B5/7278 A61B5/7405 A61B5/742 A61B5/7475 H05K999/99		
优先权	60/657596 2005-03-01 US 60/657759 2005-03-01 US 60/657268 2005-03-01 US 60/657281 2005-03-01 US		
其他公开文献	EP1860994A1		
外部链接	<a href="#">Espacenet</a>		

摘要(译)

本发明涉及一种在患者监护仪上显示生理参数的彩色编码指示的方法，该方法包括无创地确定第一生理参数的至少一个测量值和第二生理参数的至少一个测量值，将第一具有第一颜色的生理参数，将第二生理参数与不同于第一颜色的第二颜色相关联，在患者监护仪上显示具有第一颜色的第一指示，第一指示指示至少一个测量值第一生理参数，并且在患者监视器上显示具有第二颜色的第二指示，第二指示指示第二生理参数的至少一个测量值。

$$I_{\lambda} = I_{0,\lambda} e^{-d_{\lambda} \cdot \mu_{a,\lambda}}$$

(1)