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**(54) PHARMACEUTICAL DOSAGES DELIVERY SYSTEM**

SYSTEM ZUR DOSIERTEN VERABREICHUNG VON ARZNEIMITTELN

SYSTÈME D'APPORT DE DOSES PHARMACEUTIQUES

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• **MELONEY, J. M.: 'An implantable microfabricated drug delivery system' PROCEEDINGS OF IMECE'03 ASME INTERNATIONAL MECHANICAL ENGINEERING CONGRESS 15 November 2003 - 21 November 2003, WASHINGTON, D.C.,**

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**Description**

## FIELD OF THE INVENTION

**[0001]** This invention relates generally to electronic devices and, more specifically, to electronic devices that are part of a communication system that uses conduction to communicate information.

## INTRODUCTION

**[0002]** Prescription medications are effective remedies for many patients when taken properly. However, studies show that on average, about 50% of patients do not comply with prescribed medication regimens. A low rate of adherence with medication regimens results in a large number of hospitalizations and admissions to nursing homes every year. In the United States alone, it has recently been estimated that costs resulting from patient non-adherence amount to over \$100 billion annually.

**[0003]** One situation where patient adherence is of particular importance is in the context of clinical studies. Non-adherence in the clinical trial setting has long-range consequences far beyond the few hundred patients who might be involved in a trial. To the extent that non-adherence occurs without a correction factor, it may have effects ranging from failure to gain FDA approval to the necessity for increasing the recommended dose beyond that which would be required of a fully compliant population. Such an elevated dose could cause a higher incidence of side effects, which in turn may lead to further non-adherence.

**[0004]** Clinical studies typically enroll patients to undergo specific drug treatment regimens with the goal of testing hypotheses related to the effects of drug treatment on medically relevant clinical endpoints. Such studies might measure, for example, the relationship between alternative drug treatments with any of a wide variety of clinical endpoints, ranging from physiological, biochemical or psychological measurements, to manifestations of disease, patient survival or quality of life. In addition, drug treatments must also be related to any observed adverse events in an effort to identify rare adverse reactions or interactions with other medications.

**[0005]** The ability to reliably correlate highly specific drug treatment regimens, including dosage and administration methods, with both efficacy and safety depends to a great extent on the certainty of knowledge that every patient has followed the prescribed treatment regimen. Monitoring of patient adherence, including the exact time of administration for medications, is therefore of great value to clinical trial sponsors as well as the pharmaceutical industry in general.

**[0006]** Therefore, what is needed is a system and method for tracking the dosage administered and the time timing of the administration.

**[0007]** Signal emitting ingestible capsules housing pharmaceutical agents are known. Such capsules typically

ly emit signals continuously or in response to an interrogation signal and are typically powered with an onboard power storage device, such as a battery, or an onboard antenna configured to receive external energy, such as RF energy, from an external power source.

**[0008]** One such capsule is described in WO 92/21307, which is essentially a series of non-digestible compartments housing a battery, medicants, a transmitter, and an actuator. The battery must be activated prior to ingestion to initiate the transmitter to emit a non-modulated signal. The signal is then used to externally track the capsule to a desired location whereby a remote trigger may be used to provide an actuating signal to cause the actuator to activate an initiator coil. The activated initiator coil causes a piston to forcibly compress the medicant compartment such that the medicant payload is excreted from the capsule through an external port. A signal decrease caused by activation of the initiator coil indicates the beginning of the dosing procedure. The occurrence of dosing is indicated by a detectable change in resonance frequency associated with the coil caused by disruption of a parallel circuit that is tripped by movement of the piston. However, battery activation and initiation of signaling occur prior to ingestion and, therefore, the occurrence of these events do not provide information with respect to dosage administration or timing of the administration.

**[0009]** Another such non-digestible capsule is described in WO 03/068061 and includes a battery, a drug delivery module that houses one or more tanks, and a base module that includes a transceiver, a toothed wheel sensor, and a microprocessor. The microprocessor is preprogrammed to monitor revolutions of the wheel and activate the drug delivery module at preprogrammed intervals. Activation of the drug delivery module actuates a piston to expel a drug dosage from a tank. The transceiver may be used to transmit imaging or environmental data to external facilities. However, similar to WO 92/21307, activation of the battery and initiation of signaling do not provide information with respect to dosage administration or timing of the administration.

## SUMMARY

**[0010]** Devices of the invention as defined in claim 1 include a carrier component and a cap configured to seal an internal volume of the carrier component, where the cap includes a communication device that encodes information in current flow. The device includes an ingestible event marker or an ionic emission module identifier that use conduction through conducting fluid in contact with the device. Devices of invention find use in preparing a pharmaceutical dosage. Additional aspects of the disclosure include dosages prepared in accordance with the methods of the invention. Dosages prepared according to embodiments of the invention find use in a variety of different applications, including clinical trials.

## BRIEF DESCRIPTION OF THE FIGURES

**[0011]**

FIG. 1A provides a partial cut-away and perspective front view of a pharmaceutical dosage delivery system according to the present invention with a current signature producing device positioned on the exterior of the delivery system.

FIG. 1B provides a partial cut-away and perspective front view of a pharmaceutical dosage delivery system according to the present invention with a current signature producing device positioned on the interior of the delivery system.

FIG. 2A provides an exploded perspective view of the pharmaceutical dosage delivery system of FIG. 1A.

FIG. 2B provides an exploded perspective view of the pharmaceutical dosage delivery system of FIG. 1B.

FIG. 3A provides a bottom view of a cap used in the pharmaceutical dosage of FIG. 1 in accordance with the present invention.

FIG. 3B provides a side view of the cap of FIG 3A.

FIG. 3C provides a perspective view of the cap of FIG 3A.

FIG. 4 provides a cross-sectional view of a pharmaceutical dosage with an over-cap according to the present invention.

## DETAILED DESCRIPTION

**[0012]** Devices of the invention include a carrier component and a cap configured to seal an internal volume of the carrier component, where the cap includes an ingestible event marker identifier. Devices of invention find use in preparing a pharmaceutical dosage. Additional aspects of the disclosure include dosages prepared in accordance with disclosed methods which do not form part of the invention. Dosages prepared according to various aspects of the invention find use in a variety of different applications, including clinical trials.

**[0013]** In describing the invention in greater detail, devices of the invention and methods for their use in preparing a pharmaceutical dosage are reviewed first, followed by a discussion of the utility of such methods, assemblies and systems involving the same. Also reviewed in greater detail below are kits for practicing the methods.

**[0014]** As summarized above, devices and methods for their use in preparing pharmaceutical dosages are provided. The term "pharmaceutical dosage" refers to a

physically discrete structure that contains a known amount of active agent, where the known amount of active agent is one that has been selected for administration to a subject at an active agent administration event. A pharmaceutical dosage therefore contains a predetermined quantity of a pharmaceutically active agent (also referred to herein simply as an "active agent"). The amount of pharmaceutically active agent that is present in the pharmaceutical dosage is calculated to be sufficient to produce a desired effect when administered to a subject at an active agent administration event. A pharmaceutical dosage produced by methods of the invention may have any of a variety of different configurations. As such, the pharmaceutical dosage may be cylindrical, spherical or elliptical in shape, or any other convenient shape. Of interest are pharmaceutical dosages that have a substantially capsule configuration, as reviewed in greater detail below.

**[0015]** Devices of the invention include a carrier component and a cap configured to seal an internal volume of the carrier component, where the cap includes an ingestible event marker identifier. These components of the devices may vary, where different aspects of these components are described in greater detail below.

**[0016]** The methods include filling a carrier component with a pharmaceutically active agent composition and then sealing the carrier component with a cap to produce the pharmaceutical dosage. The carrier component is a container that holds an amount of pharmaceutically active agent composition. Depending on the particular nature of the pharmaceutically active agent composition (described in greater detail below), the carrier component may be configured to hold a variety of types of compositions, including liquids and solids, such as powders, tablets, coated particulate compositions, pellets, beads and spherules. While the volume of the active agent that the carrier is configured to hold may vary, in some instances the carrier may be configured to a quantity of active agent ranging from 0 to 1 g, such as 0 to 100 mg and including 0 to 5 mg. The carrier component may have a variety of different configurations. Examples of carrier component configurations include, but are not limited to partial box shapes, partial spherical shapes, partial ovoid shapes, partial conical shapes, etc.

**[0017]** One carrier component configuration of interest is a partial-capsule configuration. Partial-capsule configurations are those configurations having a first, open end and a second, closed end, where the open and closed ends are separated by a distance sufficient to provide a desired internal volume to the carrier component. Partial-capsule configurations finding use may have a variety of different cross-sectional configurations, where the cross-sectional configuration is the shape defined by the walls of the carrier component at the open end. Cross-sectional configurations of interest include, but are not limited to circular, rectangular, triangular, square and oval, as well as irregular cross sectional configurations.

**[0018]** Partial-capsule configured carrier components

of the invention may have varied dimensions, as desired. In some instances, the length of the carrier component ranges from 1 mm to 50 mm, such as 5 mm to 30 mm and including 10 mm to 20 mm. The outer diameter of the carrier component may vary, ranging in some instances from 1 mm to 30 mm, such as 5 mm to 20 mm and including 5 mm to 10 mm. The inner diameter of the carrier component may also vary, ranging from 0.5 mm to 29.99 mm, such as 3.0 mm to 19.99 mm and including 3.0 mm to 9.99 mm. The walls of the carrier component may vary, so long as they are sufficiently thick to hold the pharmaceutically active agent composition, where in some instances the walls range in thickness from 0.01 mm to 2 mm, such as 0.01 mm to 0.2 mm and including 0.01 mm to 0.1 mm. The dimensions may be constant or variable in the carrier component, as desired. For example, the inner diameter may be constant along the length of the capsule or may vary.

**[0019]** Carrier components of the invention, such as partial-capsule configured carrier components, may be fabricated from any convenient material using any convenient protocol. Materials of interest from which the carrier components may be fabricated include physiologically acceptable polymeric materials that are used in conventional pharmaceutical capsule dosages. The materials may be clear or opaque, and may be colored as desired. Of interest are both rigid and elastic materials.

**[0020]** Suitable polymers from which carrier components of the invention may be fabricated include, but are not limited to: gelatins, polyvinyl alcohol (PVA); natural and synthetic polysaccharides, including pullulan, carrageenan, xanthan, chitosan agar gums, and cellulosic materials, such as carboxymethylcellulose, hydroxypropylmethylcellulose (HPMC), methylcellulose, hydroxyethylcellulose, hydroxyethyl methylcellulose, hydroxypropylcellulose; polyethylene glycols (PEGs), polyethylene oxides (PEOs), mixtures of PEGs and PEOs; acrylic and methacrylic acid based polymers, such as EUDRAGIT E™, EUDRAGIT L™ and/or EUDRAGIT S™ methacrylic acid polymers), EUDRAGIT RL™ and/or EUDRAGIT RS™ ammonium methacrylate copolymers; povidone (polyvinyl pyrrolidone), polyglycolysed glycerides (such as GELUCIRE 44/14™, GELUCIRE 50/02™, GELUCIRE 50/13™ and GELUCIRE 53/10™ polymers); carboxyvinyl polymers (such as CARBOPOL™ polymers); polyoxyethylene-polyoxypropylene copolymers (such as POLOXAMER188™ polymer); and the like.

**[0021]** The surface of the carrier component may be smooth or comprised of variegations and/or grooves arranged in any pattern. Where desired, the carrier component has compartments or partitions. The carrier component may have multiple compartments, such that each compartment has different active agent release characteristics, or contains a different pharmaceutically active agent composition, for example as described in U.S. Patent Nos. 4,738,724; 5,672,359 and 5,443,461.

**[0022]** The carrier components may be fabricated using any convenient protocol, including molding, etc. Fab-

rication protocols of interest include, but are not limited to, those described in U.S. Patent Nos.: 5,705,189; 4,576,284; 4,591,475; 4,655,840; 4,738,724; 4,738,817 and 4,790,881. Alternatively, the carrier component may be obtained from a commercial vendor, such as Qualicaps Inc., Whitsett NC.

**[0023]** In the disclosed methods, the carrier component may be filled with a variety of different types of pharmaceutically active agent compositions. The protocol that is employed to fill the carrier component may vary depending on the nature of the pharmaceutically active agent composition. For example, flowable compositions such as liquids and solids (particulate and spherule compositions being examples of flowable solids) may be poured into the internal space of the carrier component, either manually, using an automated device, or a combination thereof, in order to fill the carrier component with the pharmaceutically active agent composition. Non-flowable solids, such as tablets or capsules, may be positioned inside of the internal volume of the carrier component, again either manually, using an automated device, or a combination thereof, in order to fill the carrier component.

**[0024]** As indicated above, the pharmaceutically active agent compositions may be solid or liquid compositions. Solid compositions of interest include, but are not limited to: powders, pellets, e.g., in the form of beads or spherules, coated granules and tablets. Liquid compositions of interest may vary, for example in terms of viscosity, color, etc. Pharmaceutically active agent compositions of the invention include a pharmaceutically active agent, either alone or in combination with a vehicle, where the vehicle may include one or more different components, such as fillers, binders, coloring agents, etc.

**[0025]** As used herein, the term "active agent" includes any compound that produces a physiological result, for example a beneficial or useful result, upon contact with a living organism, such as a human. Active agents are distinguishable from such vehicle components such as fillers, binders, coloring agents, etc. The active agent may be any molecule that is capable of modulating a biological process in a living subject. In some instances, the active agent may be a substance used in the diagnosis, treatment, or prevention of a disease or as a component of a medication. Broad categories of active agents of interest include, but are not limited to: cardiovascular agents; pain-relief agents, e.g., analgesics, anesthetics, anti-inflammatory agents, etc.; nerve-acting agents; chemotherapeutic (e.g., antineoplastic) agents; etc. Active agents of interest are further disclosed in PCT Application Serial No. US2006/016370 published as WO 2006/116718.

**[0026]** The pharmaceutically active agent composition may further include a vehicle component, as mentioned above. Vehicle components may include one or more constituents, including but not limited to fillers, binders, disintegrants, coloring agents, etc. Vehicle components of interest are further reviewed in PCT Application Serial

No. US2006/016370 published as WO 2006/116718. Additional disclosure of components that can be present in compositions of the invention can be found in Remington's Pharmaceutical Sciences, Mace Publishing Company, Philadelphia, Pa., 17th ed. (1985).

**[0027]** In some instances, the methods may include providing a filler composition that is separate from the active agent composition in the carrier component. For example, in some instances the carrier component is filled with both a pharmaceutically active agent composition and a distinct filler composition, where the filler composition may be included for a variety of different purposes. One type of filler composition of interest is one that imparts to the pharmaceutical dosage composition a density that is greater than stomach fluid. Accordingly, filler compositions of interest are ones that impart to the pharmaceutical dosage composition a density that is 0.8 or greater, such as 1.0 or greater and including 1.2 or greater. Any convenient material may be employed as a filler composition, including the materials described as vehicle components, above.

**[0028]** The filler may also be included to fill any void space present when a device or identifier, such as an current control device, such as an ingestible event marker (IEM, which is also known as an ionic emission module) identifier is placed inside of the carrier components. The identifier component of the dosages provides for a number of advantages. The presence of the identifier allows one to monitor the exact time and frequency of medication administration, as well as patient response. This information obtainable by use of the methods and dosages of the invention can be exploited in a number of settings, such as, for example, in improving the overall quality and accuracy of clinical studies. Using such information, one can readily identify members of the clinical trial who comply with a treatment regimen and exclude those that do not in order to obtain more accurate data regarding efficacy of a given active agent. Such information can also be combined with various types of physiological data in order to obtain more comprehensive information regarding the effect of a given active agent.

**[0029]** The disclosed methods also find use with pharmacists, who can prepare patient customized dosages that include an IEM, even if the original manufacturers of the active agent of interest does not provide dosages that include an IEM. An IEM is a device that is dimensioned to be ingestible and includes a conductance control module and a partial power source that is completed upon contact with conducting fluid. As the IEMs are dimensioned to be ingestible, they are sized so that they can be placed in a human mouth and swallowed. In some instances, IEMs of the invention have a longest dimension that is 30 mm or less, such as 20 mm or less, including 5 mm or less. As such, any pharmaceutical composition currently available can be associated with an IEM using components of the invention.

**[0030]** Following placement of the pharmaceutically active agent composition (and any optional filler compo-

sition as desired) into the internal volume of the carrier component, the resultant filled carrier component is then sealed with a cap. A cap is a structure configured to mate with the open end of a carrier component in a sealing relationship, such that when the cap is associated with the open end of the carrier component, an internal volume of the carrier component and contents thereof (the pharmaceutically active agent composition) are sealed from the external environment of the dosage structure defined by the carrier and cap, such that gases and liquids may not readily pass between the external and internal environments of the dosage structure. The cap may be fabricated from any suitable material, including the materials described above in connection with the carrier component. In some instances, the cap is fabricated from microcrystalline cellulose, croscarmellose sodium and magnesium stearate.

**[0031]** Caps of the invention include one or more IEM identifiers. The one or more IEM may be present at a variety of different locations of the cap, including internal locations and external locations. Internal locations include areas defined inside of the cap that are configured to receive the IEM. External locations include outer and inner surfaces. Outer surfaces of the cap are those surfaces that face the external environment of the cap when the cap is in a sealing relationship with the carrier component. The outer surface may be a side surface of the cap or a top surface of the cap, as desired. Inner surfaces of the cap are those surfaces that face the internal volume defined by the carrier component and cap when the cap is in a sealing relationship with the carrier component. A given cap may include a single IEM or two or more IEMs, such as three or more ingestible event markers. The one or more IEMs are stably associated with the cap. As such, the identifiers are fixed to a location of the cap, such as an outer surface of the cap, for example by use of an adhesive. Adhesives of interest include, but are not limited to: sugar and cellulosic adhesives, protein adhesives such as zein or casein, silicone adhesives, polymeric adhesives, including acrylic and methacrylic adhesives, shellac, and the like.

**[0032]** IEMs of interest are identifiers that communicate information through production of a unique current signature that flows through a conducting environment, such as a conducting fluid, upon contact of the IEM with a target physiological location (or locations). The IEMs may vary depending on the particular embodiment and intended application of the composition, as long as they are activated (turned on) upon contact with a target physiological location, such as the stomach fluid or intestinal fluid. As such, an IEM may be an identifier that produces a unique current signature encoded with information when activated at a target site, for example when the IEM contacts a target body site. The IEM may be any component or device that is capable of providing a detectable signal following activation. IEMs according to various aspects of the present invention comprise a control unit for producing a unique current signature. The IEM may be

configured to produce the unique current signature once the composition comes into contact with a physiological target site. Depending on the embodiment, the target physiological site or location may vary, where representative target physiological sites of interest include, but are not limited to: a location in the gastrointestinal tract, such as the mouth, esophagus, stomach, small intestine, large intestine, etc. IEMs may be configured to be activated upon contact with fluid at the target site, e.g., stomach fluid, regardless of the particular composition of the target site. Where desired, the identifier may be configured to be activated by interrogation, following contact of the composition with a target physiological site. The IEM may be configured to be activated after a specific period of time, wherein the target site is reached after a specified period of time.

**[0033]** Depending on the needs of a particular application, the information obtained from the IEM may be generic, such that the information merely identifies that the composition has contacted the target site. Alternatively, the information may be unique, which in some way uniquely identifies that a particular IEM from a group or plurality of different markers in a batch of dosages has contacted a target physiological site. As such, the IEM may be one that, when employed with a batch of dosages, emits a current signature which cannot be distinguished from the current signature emitted by the IEM of any other dosage member of the batch. Alternatively, each IEM of the batch may emit a unique signal, at least with respect to all the other IEMs of the batch. In these instances, each IEM of the batch produces a current signature that uniquely identifies that particular IEM with respect to all other IEMs in the batch. The IEM may emit a unique current signature that is a universally unique current signature (where such a current signature may be analogous to a human fingerprint which is distinct from any other fingerprint of any other individual and therefore uniquely identifies an individual on a universal level). The current signature may either directly convey information about a given event, or provide an identifying code, which may be used to retrieve information about the event from a database, i.e., a database linking identifying codes with compositions.

**[0034]** The duration of the current generation period of the IEM may vary, in accordance with the teachings of the present invention, from 0.1  $\mu$ sec to 48 hours or longer, such as from 0.1  $\mu$ sec to 24 hours or longer, such as from 0.1  $\mu$ sec to 4 hours or longer, such as from 1 sec to 4 hours, including from 1 minute to 10 minutes. Depending on the given embodiment, the IEM may produce the same information encoded in the current signature one time; alternatively, the IEM may be configured to produce the current signature with the same information (identical), two or more times, where the collection of discrete identical current signatures may be collectively referred to as a redundant signal.

**[0035]** In addition to producing a unique current signature, in accordance with other aspects of the present in-

vention, the IEM may be configured to generate a variety of different types of signals, including but not limited to: RF signals, magnetic signals, acoustic signals, etc.

**[0036]** The IEM may vary depending on the particular embodiment and intended application of the composition so long as they are activated (i.e., turned on) upon contact with a target physiological location, such as the stomach. The IEM includes a partial power source that is completed by a conducting fluid, such as stomach acid, and a conductance control unit. Examples of different types of IEMs of interest include, but are not limited to, those described in PCT application serial no. PCT/US2006/016370 published as WO/2006/1 16718; PCT application serial no. PCT/US2007/082563 published as WO/2008/052136; PCT application serial no. PCT/US2007/024225 published as WO/2008/063626; PCT application serial no. PCT/US2007/022257 published as WO/2008/066617; PCT application serial no. PCT/US2008/052845 published as WO/2008/095183; PCT application serial no. PCT/US2008/053999 published as WO/2008/101 107; PCT application serial no. PCT/US2008/056296 published as WO/2008/1 12577; PCT application serial no. PCT/US2008/056299 published as WO/2008/1 12578; PCT application serial no. PCT/US2008/077753; and U.S. patent application serial no. 12/564,017 filed September 21, 2009.

**[0037]** The cap may have a variety of different configurations so long as it is configured to seal the open end of the carrier component when it is associated with the open end of the carrier component. The cap may have a variety of different configurations which allow it to seal the open end of the carrier component when associated with the open end of the carrier component. In some instances, the cap has a sealing portion that is in physical communication with the open end of the carrier housing to seal the cavity containing the pharmaceutical agent, and the sealing portion includes interlocking elements which operate in conjunction with mating elements of the open end of the carrier component to seal the open end of the carrier component. Examples of interlocking elements are screw threads and snap-fit elements. Alternatively, the cap may have a region or end that is configured to pressure fit inside of the carrier component and seal the contents of the carrier component. An example of such a configuration is where the cap has an end made up of a rigid material, where the configuration of the end is slightly larger than the open end of the carrier component. Where the open end of the carrier component is made of an elastomeric material, the rigid end of the cap can be pressure fit into the open end of the carrier by stretching the open end of the carrier. When any stretching force is removed from the open end of the carrier, the open end of the carrier will then comply with the rigid end of the cap in a sealing relationship. Alternatively, the cap may include a compressible end which has a certain amount of compliancy. This compliancy is sufficient to impart to the cap the ability to pressure fit the pliable end of the cap inside the open end of the carrier component

by compressing the compressible end to produce a compressed end, placing the compressed end of the cap in the open end of the carrier component and then removing the compressive force. When the compressed end expands as a result of removal of the compressive force, the compressed end conforms to the configuration of the open end of the carrier component in a sealing relationship to seal the contents of the carrier component inside of the carrier component.

**[0038]** A cap with a compressible end can be provided in a number of different ways. One type of compressible end is an end that is fabricated from a compressible material. Compressible materials of interest are pliable. Alternatively, the compressible end may include one or more cut-outs that impart compressibility to the compressible end.

**[0039]** Where desired, the cap may be secured to the open end of the carrier component with an adhesive, where examples of suitable adhesives are provided above. As such, the cap may be glued onto the open end of the carrier component in order to seal the open end of the carrier component.

**[0040]** In some instances, passageways or analogous structures are provided in the carrier and/or cap which facilitate liquid penetration of the dosage form, dissolution of the carrier components and/or reduce buoyancy of the dosage form. When present, such holes may range from 10<sup><~3></sup> to 5 mm in diameter, such as 0.1 to 2 mm in diameter.

**[0041]** Referring now to FIGS. 1A and 2A, a pharmaceutical dosage carrier system 10 includes a cap 20 and housing or housing 50. The housing 50 of the system 10 defines a cavity and includes an open end 60 and a closed end 70. The closed end 70 has a partially-planer base with side walls extending from the base in an upward direction, finishing with an open mouth at the open end 60 to define the cavity therein. The closed end 70 may also be a rounded structure, such as a hemispherical end wall, among other configurations, and have a conical configuration, etc.

**[0042]** The system 10 includes an engagement area 65 on the inner wall of the housing 50. The engagement area 65 can be engaged with the cap 20 when the cap 20 is inserted into the open end 60 of the housing 50 in a manner sufficient to produce a seal between the housing 50 and the cap 20. The cap 20 and housing 50 sizes are chosen such that there is contact between the external wall of the cap 20 and the internal wall of the engagement area 65 of the housing 50.

**[0043]** As reviewed above, the system 10 may be filled with a pharmaceutically active agent composition and/or a filler composition. In accordance with one aspect of the present invention, the system 10 is filled with a pharmaceutically active agent composition and two filler compositions that are in the form of tablets. As such, the housing 50 is filled with a pharmaceutically active agent tablet 30 and two filler compositions 35 and 37. Although shown in a specific order within the cavity defined by the housing

50, the scope of the present invention is not limited by the relative positions or the order of the tablet 30 and the filler compositions 35 and 37. For example, the tablet 30 may be positioned at the location of filler composition 37 as shown in Fig. 1A. Additionally, the orientation of the tablet 30 and the filler composition 35 and 37 may be flipped to better accommodate assembly of the system 10, as shown in FIGS. 1B and 2B, and the scope of the present invention is not limited thereby. At least one of the filler compositions 35 and 37 are fabricated from a material such that impart a density to the overall system 10. In accordance with one aspect of the present invention, the density may be greater than the density of the environment that the system 10 enters or is introduced to, such as stomach fluid. Thus, either one of the filler compositions 35 and 37 can be used to alter the buoyancy of the system 10; the other filler composition may be used to prevent movement of the tablet 30 and the other filler composition within the cavity defined by the housing 50. In accordance with another aspect of the present invention, both of the filler compositions may be used to alter the buoyancy of the system 10. In accordance with the teaching of the present invention, either one of filler compositions may be replaced by a pharmaceutical agent, such that the system 10 includes two (or more?) different pharmaceutically active agents that are released into the surrounding environment at different times or at the same times.

**[0044]** Referring now to FIGS. 1A and 1B, in assembling the system 10, the pharmaceutically active agent, such as the tablet 30, and the two filler compositions 35 and 37 are positioned inside of housing 50 as shown. This positioning step may be accomplished manually or by automatic methods, such as through the use of an assembly machine, remote robot, or other automated device. Following placement of the tablet 30 and the filler compositions 35 and 37 into the housing 50, the open end 60 of the housing 50 is sealed with the cap 20 to seal the system 10. Sealing the open end 60 of the housing 50 with the cap 20 may be accomplished manually or by automatic methods, such as through the use of an assembly machine, remote robot, or other automated device.

**[0045]** As shown in FIGS. 1A and 2A, the cavity defined by the housing 50 that contains the tablet 30 as well as the filler compositions 35 and 37 is sealed with the cap 20. The cap 20 may be pressure-fit inside of the open end 60 of the housing 50. In accordance with another aspect of the present invention, the cap 20 may be glued to the engagement area 65.

**[0046]** Referring now to FIGS. 1A and 2A, the cap 20 includes a device 40, such as an IEM, on a top-outer surface thereof. The device 40 is secured to the upper surface of the cap 20 through the use of a suitable securing method. For example, in accordance with one aspect of the present invention the device 40 is glued to the cap 20 using a suitable adhesive. Alternatively, as shown in FIGS 1B and 2B, the device 40 maybe secured

to a bottom-inner surface of the cap 20 such that when the cap 20 is positioned within the cavity of the housing 50, the device 40 is sealed therein and protected from contact with the surrounding environment that the system 10 is introduced to until the cap 20 is released from the housing 50.

**[0047]** In accordance with another aspect of the present invention, the device 40 includes a virtual dipole element as described in PCT application serial no. PCT/US2008/077753. In accordance with other aspect of the present invention, the device 40 may not be visible.

**[0048]** Referring now to FIGS. 1A and 2A, the cap 20 includes an insertion portion 80 that is fitted into the open end 60 of the housing 50, as described above. The insertion portion 80 is opposite the surface on which the device 40 is positioned. As shown, the insertion portion 80 defines at least one cut-out portion 90 that allows the insertion portion 80 to be fitted inside of the open end 60. The open end 60 may be malleable to stretch over and pressure fit onto the insertion portion 80 and provide for a secure fit. As such, the cap 20 may be pinched to fit into the open end 60 of the housing 50 when used to seal the insertion portion 80 into the open end 60.

**[0049]** Referring now to FIGS. 1B and 2B, the cap 20 includes an insertion portion 80 that is fitted into the open end 60 of the housing 50, as described above. The insertion portion 80 is located proximal to the bottom surface of the cap 20. The bottom surface of the cap 20 is shaped to receive the device 40 that is positioned on and secured to the bottom surface. As shown, the insertion portion 80 defines a plurality of cut-out portions 90 that allows the insertion portion 80 to be fitted inside of the open end 60. However, the scope of the present invention is not limited by the shape or the number of cut-out portions on the bottom surface of the cap 20. The open end 60 may be malleable to stretch over and pressure fit onto the insertion portion 80 and provide for a secure fit. Alternatively and in accordance with another aspect of the present invention, the open end 60 may be rigid and tapered (not shown) to matingly receive a tapered insertion portion (not shown) of the cap 20, wherein the tapered portion or the open end 60 and the tapered insertion portion of the cap 20 are glued together. As such, the cap 20 may be pressed and glued into the open end 60 of the housing 50 to secure the cap 20 to housing 50.

**[0050]** Referring now FIGS. 3A, 3B, and 3C, the cap 20 includes the insertion portion 80. In accordance with one aspect of the present invention, the insertion portion 80 defines four channels or cut-outs 92, 94, 96 and 98. Each cut-out has a near-crescent shape, as shown. However, the cut-outs 92, 94, 96, and 98 may have any suitable shape that facilitates fitting of the cap 20 into the open end 60, such as a polygonal shape. As shown, the insertion portion 80 of the cap 20 includes a circumferential annular beveled ridge.

**[0051]** In some instances, the cap 20 that is secured to the end of the housing 50 may be covered by an over-cap component. The over-cap component may be fabri-

cated from a variety of materials, such as any of the materials employed for the carrier component. The over-cap may be fabricated from an opaque material so as to hide the presence of a device 40 as well as prevent contact with the surrounding during packaging and handling. The over-cap component may be elastomeric, for example to provide for a secure fit over the cap that is in sealing relation with the carrier component.

**[0052]** Referring now to FIG. 4, in accordance with another aspect of the present invention a pharmaceutical dosage system 130 includes an over-cap 132. The pharmaceutical dosage system 130 includes a carrier component 140 sealed with a cap 134. The cap 134 includes a device 136, such as a current signature production device or IEM, on an outer surface thereof. Positioned over cap 134 is the over-cap 132. The over-cap 132 is secured to the carrier component 140 as shown; this prevents contact between the device 136 and conducting fluid once the pharmaceutical dosage system 130 is ingested. Once the over-cap 132 is released from the carrier component 140, the device 136 comes into contact with the surrounding environment and if that environment includes a conducting fluid, such as stomach fluid, then the device 136 is activated and produces a current signature that can be detected and decoded to retrieve information.

**[0053]** Where desired, the methods of preparing the dosage delivery system may further include preparing placebo pharmaceutical dosages. Placebo pharmaceutical dosages may be prepared in a manner analogous to the preparation of dosages that include a pharmaceutically active agent, with the exception that a pharmaceutically active agent is not placed inside of a carrier component. Instead, a vehicle composition that lacks an active agent, for example as described above, is placed inside of the carrier component and then sealed with the cap. Methods where placebo dosages are prepared include methods in which the pharmaceutical dosages are to be employed in clinical trials.

**[0054]** In accordance with yet another aspect of the present disclosure, the methods of preparing a dosage delivery system may further include preparing dosages having a device within the carrier, e.g., either alone or in combination with a filler. Such aspects may facilitate, among other applications, marking of an ingestion event of the dosage delivery system via production of a unique current signature.

**[0055]** In accordance with another aspect of the present invention, two different pharmaceutical agents may be placed within the housing 50 and separated by a filler composition. This physical separation is beneficial in instances where to different pharmaceutical agents must be mixed in solution to become active. Thus, as the housing 50 is dissolved, the two separate pharmaceutical agents are released into the surrounding fluid, such as the stomach fluid. This causes the two previously separated pharmaceutical agents to come into contact and combine, thereby allowing accurate delivery and combi-

nation of two different pharmaceutical agents at a target site.

**[0056]** Further aspects include methods of using the pharmaceutical dosages that are produced according to methods as described above. Generally, methods of the invention will include administering one or more pharmaceutical dosages to a subject, for example by having a subject ingest a pharmaceutical dosage of the invention. The dosages may be administered to a variety of different types of subjects. Generally such subjects are "mammals" or "mammalian," where these terms are used broadly to describe organisms which are within the class mammalia, including the orders carnivore (for example dogs and cats), rodentia (for example mice, guinea pigs, and rats), and primates (for example humans, chimpanzees, and monkeys). Following ingestion, a unique current signature is produced by an IEM and detected, for example with a receiver, such as described in PCT application serial no. PCT/US2006/016370 published as WO/2006/1 16718; PCT application serial no. PCT/US2007/082563 published as WO/2008/052136; PCT application serial no. PCT/US2007/024225 published as WO/2008/063626; PCT application serial no. PCT/US2007/022257 published as WO/2008/066617; PCT application serial no. PCT/US2008/052845 published as WO/2008/095183; PCT application serial no. PCT/US2008/053999 published as WO/2008/101 107; PCT application serial no. PCT/US2008/056296 published as WO/2008/1 12577; PCT application serial no. PCT/US2008/056299 published as WO/2008/1 12578; PCT application serial no. PCT/US2008/077753; U.S. patent application serial no. 61/251 ,088 filed October 13, 2009; and PCT patent application serial no. PCT/US2009/068128 filed December 15, 2009.

**[0057]** Methods of preparing pharmaceutical dosages and administering the same to subjects, for example as described above, find use in a variety of different applications. One application of interest is the use of the identifiers of the dosages as IEMs. Pharmaceutical dosages can be used in both therapeutic and non-therapeutic applications, such as reviewed in PCT application serial no. PCT/US2006/016370 published as WO/2006/1 16718; PCT application serial no. PCT/US2007/082563 published as WO/2008/052136; PCT application serial no. PCT/US2007/024225 published as WO/2008/063626; PCT application serial no. PCT/US2007/022257 published as WO/2008/066617; PCT application serial no. PCT/US2008/052845 published as WO/2008/095183; PCT application serial no. PCT/US2008/053999 published as WO/2008/101 107; PCT application serial no. PCT/US2008/056296 published as WO/2008/1 12577; PCT application serial no. PCT/US2008/056299 published as WO/2008/1 12578; and PCT application serial no. PCT/2008/077753.

**[0058]** Applications of interest include automatic detection and identification of pharmaceutical agents actually delivered into the body, as may be done in: (1) monitoring patient adherence with prescribed therapeutic

regimens; (2) tailoring therapeutic regimens based on patient adherence; (3) monitoring patient adherence in clinical trials; (4) monitoring usage of controlled substances; and the like. Each of these different illustrative applications is reviewed in greater detail in PCT application serial no. PCT/US2006/016370 published as WO/2006/116718; PCT application serial no. PCT/US2007/082563 published as WO/2008/052136; PCT application serial no. PCT/US2007/024225 published as WO/2008/063626; PCT application serial no. PCT/US2007/022257 published as WO/2008/066617; PCT application serial no. PCT/US2008/052845 published as WO/2008/095183; PCT application serial no. PCT/US2008/053999 published as WO/2008/101107; PCT application serial no. PCT/US2008/056296 published as WO/2008/112577; PCT application serial no. PCT/US2008/056299 published as WO/2008/112578; and PCT application serial no. PCT/US2008/077753.

**[0059]** In certain aspects, the methods of making pharmaceutical dosages of the invention are employed in clinical trials. Clinical trials in which the methods and compositions include multi-patient studies that are conducted to allow safety and efficacy data to be collected for a new pharmaceutically active agent. Examples of clinical trials include studies where investigators enroll healthy volunteers and/or patients into small pilot studies initially, followed by larger scale studies in patients that often compare the new product with a currently prescribed treatment. Furthermore, clinical trials may also compare the active agent of interest with a placebo composition. In these instances, placebos may be produced in a manner analogous to the exemplary methods of producing pharmaceutical dosages, with the only difference being that a pharmaceutically active agent composition is not sealed the carrier component. As positive safety and efficacy data are gathered in a given clinical trial, the number of patients may be increased. Clinical trials can vary in size from a single center in one country to multi-center trials in multiple countries.

**[0060]** Performing clinical trials with the disclosed pharmaceutical provides a number of advantages. One advantage is that the clinical trial manager (the entity who is running the clinical trial) can use standard carrier components and caps and customize these as needed with a given pharmaceutically active agent composition.

**[0061]** Also provided are systems that include one more pharmaceutical dosages, as described above. In addition to the pharmaceutical dosages of the invention, the systems may include body-associated signal receivers for detecting changes in voltage potential that represent receiving encoded information from a pharmaceutical dosage carrier in accordance with the teaching of the present invention. Body-associated receivers of interest include those described in PCT/US2008/052845 published as WO/2008/095183 and PCT/US2006/016370 published as WO/2006/116718. As described in these incorporated applications, the receivers may be implanted or on a body surface of a pa-

tient. The systems may further include additional data relay and/or processing components, such as wireless communication devices (such as cell phones); data processors as may be found in computers and information systems, etc.

**[0062]** Also provided are kits for practicing the subject methods. Kits may include one or more carrier components and associated caps of the invention, as described above. The carrier components and associated caps of the kits will be equipped to receive a dosage amount of one or more pharmaceutically active agent compositions to be sealed therein; such as pharmaceutically active agent compositions being provided separately from the instant kits. Where desired, the kits may also include one or more filler compositions. A given kit may include sufficient carrier components and caps to make 1 or more, including 5 or more, such as 50 or more, 100 or more, 1000 or more, 5000 or more, or 10000 or more pharmaceutical dosages.

**[0063]** The subject kits may also include instructions for how to practice the subject methods using the components of the kit. The instructions may be recorded on a suitable recording medium or substrate. For example, the instructions may be printed on a substrate, such as paper or plastic, etc. As such, the instructions may be present in the kits as a package insert, in the labeling of the container of the kit or components thereof (i.e., associated with the packaging or sub-packaging) etc. In other embodiments, the instructions are present as an electronic storage data file present on a suitable computer readable storage medium, e.g. CD-ROM, diskette, etc. In yet other embodiments, the actual instructions are not present in the kit, but means for obtaining the instructions from a remote source, e.g. via the internet, are provided. An example of this embodiment is a kit that includes a web address where the instructions can be viewed and/or from which the instructions can be downloaded. As with the instructions, this means for obtaining the instructions is recorded on a suitable substrate.

**[0064]** Some or all components of the subject kits may be packaged in suitable packaging to maintain sterility. Where desired, the components of the kit are packaged in a kit containment element to make a single, easily handled unit, where the kit containment element may be a box or analogous structure and may or may not be an airtight container.

**[0065]** It is to be understood that this invention is not limited to particular embodiments described, as such may vary. It is also to be understood that the terminology used herein is for the purpose of describing particular embodiments only, and is not intended to be limiting, since the scope of the present invention will be limited only by the appended claims.

**[0066]** Where a range of values is provided, it is understood that each intervening value, to the tenth of the unit of the lower limit unless the context clearly dictates otherwise, between the upper and lower limit of that range and any other stated or intervening value in that stated

range, is encompassed within the invention. The upper and lower limits of these smaller ranges may independently be included in the smaller ranges and are also encompassed within the invention, subject to any specifically excluded limit in the stated range. Where the stated range includes one or both of the limits, ranges excluding either or both of those included limits are also included in the invention.

**[0067]** Unless defined otherwise, all technical and scientific terms used herein have the same meaning as commonly understood by one of ordinary skill in the art to which this invention belongs. Although any methods and materials similar or equivalent to those described herein can also be used in the practice or testing of the present invention, representative illustrative methods and materials are now described.

**[0068]** It is noted that, as used herein and in the appended claims, the singular forms "a", "an", and "the" include plural referents unless the context clearly dictates otherwise. It is further noted that the claims may be drafted to exclude any optional element. As such, this statement is intended to serve as antecedent basis for use of such exclusive terminology as "solely," "only" and the like in connection with the recitation of claim elements, or use of a "negative" limitation.

**[0069]** Certain ranges have been presented herein with numerical values being preceded by the term "about." The term "about" is used herein to provide literal support for the exact number that it precedes, as well as a number that is near to or approximately the number that the term precedes. In determining whether a number is near to or approximately a specifically recited number, the near or approximating unrecited number may be a number which, in the context in which it is presented, provides the substantial equivalent of the specifically recited number.

**[0070]** As will be apparent to those of skill in the art upon reading this disclosure, each of the individual embodiments described and illustrated herein has discrete components and features which may be readily separated from or combined with the features of any of the other several embodiments without departing from the scope or spirit of the present invention. Any recited method can be carried out in the order of events recited or in any other order which is logically possible.

**[0071]** Although the foregoing invention has been described in some detail by way of illustration and example for purposes of clarity of understanding, it is readily apparent to those of ordinary skill in the art in light of the teachings of this invention that certain changes and modifications may be made thereto without departing from the scope of the appended claims.

## Claims

1. A pharmaceutical delivery system for tracking delivery parameters, the system comprising:

a carrier housing (50,140) having a closed end (70) and an open end (60), wherein the carrier housing defines a cavity;

a pharmaceutical agent positionable or positioned within the cavity of the carrier housing; and

a cap (20,134) comprising a top end and a bottom end, wherein the bottom end includes a sealing portion that is in physical communication with the open end of the carrier housing to seal the cavity containing the pharmaceutical agent; **characterized in that** the pharmaceutical delivery system further includes

a device (40,136) associated with the system, wherein the device is configured to produce an identifiable current signature for communicating information regarding delivery of a dosage of the pharmaceutical agent,

wherein the device is a current control device secured to the cap and configured for producing a unique current signature, wherein the current control device comprises:

a conductance control module for producing an identifiable current signature; and

a partial power source comprising a first material and a second material insulated from one another and each of the first material and the second material being electrically coupled to the conductance control module, the partial power source of the current control device being configured to produce a voltage potential when the first material and the second material are electrically coupled through a conducting fluid in contact therewith and the voltage potential being used to activate the conductance control module to produce the identifiable current signature.

2. The system as claimed in claim 1, wherein the sealing portion is an insertion portion (80).
3. The system as claimed in claim 1, wherein the current control device is an ingestible event marker (IEM) device.
4. The system of claim 1, wherein the device is secured to the top end of the cap such that the device is able to come into contact with the surrounding environment as the housing (50,140) comes into contact with the surrounding environment.
5. The system of any of the preceding claims, wherein the sealing portion defines at least one channel (92,94,96,98) that allows the cap (20,134) to be pressure fitted into the open end (60) of the carrier housing (50,140) and/or wherein the sealing portion is secured to the open end (60) of the carrier housing

using an adhesive and/or wherein the sealing portion comprises a compressible end, preferably an end fabricated from a compressible material, such that it may be pressure fitted into the open end (60) of the carrier house (50, 140).

6. The system of any of claims 1-5, wherein the device is secured to the bottom end such that the device comes into contact with the surrounding environment after the system is ingested and the cap separates from the carrier housing.
7. The system as claimed in any of the preceding claims, comprising:
  - a material positioned within the cavity of the housing (50,140) for altering the buoyancy of the system.
8. The system of claim 1, wherein the current control device is secured to the top end of the cap such that the first and second materials of the partial power source of the current control device come into contact with the conducting fluid at about the same time that the housing comes into contact with the conducting fluid and, hence, the conductance control module of the current control device is activated upon contact with a conducting body fluid; and/or wherein the current control device (40,136) is secured to the top end of the cap (20,134) and wherein the system further comprises an over-cap (132) positioned over the top end of the cap (20,134), such that the over-cap prevents contact of the conducting body fluid with the first and second materials of the partial power source of the current control device until the over-cap (132) dissolves, which causes a delay between the time of introduction of the system to the environment and activation of the conductance control module and thereby delaying generation of the identifiable current signature; and/or wherein the current control device is secured to the bottom end of the cap such that the first and second materials of the partial power source of the current control device come into contact with the surrounding environment after the cap is separated from the housing thereby delaying the conductance control module of the current control device from producing the identifiable current signature.
9. The system as claimed in any of the preceding claims, wherein the cap (20,134) includes a tapered portion at the bottom end and the housing (50,140) includes a tapered portion at the open end such that the tapered portions are male-female mated and glued together thereby causing the cap to be secured into the open end of the housing to seal the cavity; and/or wherein the cap is mechanically fitted to the open end of the housing to seal the cavity of the housing and/or further comprising a pharmaceutical agent positioned within the cavity of the housing

(50,140) and/or wherein the apparatus has a composition that imparts to the device a density that is greater than stomach fluid.

10. The system as claimed in any of the preceding claims, the system comprising a carrier comprising: a dissolvable housing that defines a cavity, wherein the housing includes an open end and a closed end and the pharmaceutical agent is positionable within the cavity defined by the housing. 5
11. The system of claim 10, wherein the device is secured to the top end of the cap such that the device contacts the conducting fluid at about the same time that the housing contacts the conducting fluid. 10
12. The system of any of claims 10 to 11, wherein the device is positioned on the top end of the cap and wherein the carrier further comprises an over-cap positioned around the cap and secured to the cap, such that the over-cap causes a delay in activation of the device by delaying contact between the device and the conducting fluid and, hence, a delay in production of the current signature. 20
13. The system of claim 12, wherein the device is secured to a bottom of the over-cap such that the device comes into contact with the conducting fluid after the housing is dissolved to the point where the cap is released thereby causing a delay in producing the current signature, and/or wherein the device is placed within the cavity defined by the housing, and/or further comprising a buoyancy altering apparatus positioned within the cavity defined by the housing. 25
14. The system as claimed in any of the preceding claims, wherein the carrier further comprises a filler composition positioned within the cavity defined by the housing to prevent movement of the pharmaceutical agent and the device within the cavity defined by the housing. 30
15. The system as claimed in any of claims 12 to 14, wherein the over-cap is glued into the open end of the housing (50) and/or mechanically secured to the open end of the housing and/or pressure fitted to the open end of the housing. 35

#### Patentansprüche

1. Ein pharmazeutisches Abgabesystem zum Verfolgen von Abgabeparametern, wobei das System Folgendes beinhaltet: 40

ein Trägergehäuse (50, 140) mit einem geschlossenen Ende (70) und einem offenen Ende

(60), wobei das Trägergehäuse einen Hohlraum definiert;

einen pharmazeutischen Wirkstoff, der in dem Hohlraum des Trägergehäuses positionierbar oder positioniert ist; und

eine Kappe (20, 134), die ein oberes Ende und ein unteres Ende beinhaltet, wobei das untere Ende einen Abdichtungsabschnitt umfasst, der physisch mit dem offenen Ende des Trägergehäuses kommuniziert, sodass der den pharmazeutischen Wirkstoff enthaltende Hohlraum abgedichtet wird, **dadurch gekennzeichnet, dass** das pharmazeutische Abgabesystem des Weiteren Folgendes umfasst: 15

ein mit dem System assoziiertes Gerät (40, 136),

wobei das Gerät konfiguriert ist, um eine identifizierbare Stromsignatur zum Kommunizieren von Informationen bezüglich der Abgabe einer Dosis des pharmazeutischen Wirkstoffs zu erzeugen, wobei das Gerät ein Stromsteuerungsgerät ist, das an der Kappe befestigt und konfiguriert ist, um eine eindeutige Stromsignatur zu erzeugen, wobei das Stromsteuerungsgerät Folgendes beinhaltet: 25

ein Leitfähigkeitssteuerungsmodul zum Erzeugen einer identifizierbaren Stromsignatur; und

eine Teilenergiequelle, beinhaltend ein erstes Material und ein zweites Material, die voneinander isoliert sind, und wobei jedes des ersten Materials und des zweiten Materials elektrisch an das Leitfähigkeitssteuerungsmodul gekoppelt ist, wobei die Teilenergiequelle des Stromsteuerungsgeräts konfiguriert ist, um ein Spannungspotential zu erzeugen, wenn das erste Material und das zweite Material durch ein leitfähiges Fluid bei Kontakt damit elektrisch gekoppelt werden, und das Spannungspotential genutzt wird, um das Leitfähigkeitssteuerungsmodul zu aktivieren, um die identifizierbare Stromsignatur zu erzeugen. 30

2. System gemäß Anspruch 1, wobei der Abdichtungsabschnitt 5 ein Einsteckabschnitt (80) ist. 45

3. System gemäß Anspruch 1, wobei das Stromsteuerungsgerät ein einnehmbares Gerät zur Ereigniskennzeichnung (IEM) ist. 50

4. System gemäß Anspruch 1, wobei das Gerät an dem oberen Ende der Kappe befestigt ist, sodass das Ge- 55

rät mit dem umgebenden Milieu in Kontakt kommen kann, wenn das Gehäuse (50, 140) mit dem umgebenden Milieu in Kontakt kommt.

5. System gemäß einem der vorhergehenden Ansprüche, wobei der Abdichtungsabschnitt mindestens einen Kanal (92, 94, 96, 98) definiert, der es der Kappe (20, 134) ermöglicht, mittels Druck in das offene Ende (60) des Trägergehäuses (50, 140) eingepasst zu werden, und/oder wobei 20 der Abdichtungsabschnitt unter Verwendung eines Klebemittels an dem offenen Ende (60) des Trägergehäuses befestigt ist und/oder wobei der Abdichtungsabschnitt ein komprimierbares Ende beinhaltet, vorzugsweise ein aus einem komprimierbaren Material gefertigtes Ende, sodass er mittels Druck in das offene Ende (60) des Trägergehäuses (50, 140) eingepasst werden kann.
6. System gemäß einem der Ansprüche 1-5, wobei das Gerät an dem unteren Ende befestigt ist, sodass das Gerät in Kontakt mit dem umgebenden Milieu kommt, nachdem das System eingenommen wurde und sich die Kappe von dem Trägergehäuse trennt.
7. System gemäß einem der vorhergehenden Ansprüche, das Folgendes beinhaltet:  
ein in dem Hohlraum des Gehäuses (50, 140) positioniertes Material zum Verändern des Auftriebs des Systems.
8. System gemäß Anspruch 1, wobei das Stromsteuerungsgerät an dem oberen Ende der Kappe befestigt ist, sodass das erste und zweite Material der Teilenergiequelle des Stromsteuerungsgeräts ungefähr zur gleichen Zeit mit dem leitfähigen Fluid 10 in Kontakt kommen, zu der das Gehäuse mit dem leitfähigen Fluid in Kontakt kommt, und somit das Leitfähigkeitssteuerungsmodul des Stromsteuerungsgeräts bei Kontakt mit einem leitfähigen Körperfluid aktiviert wird; und/oder wobei das Stromsteuerungsgerät (40, 136) an dem oberen Ende der Kappe (20, 134) befestigt ist und wobei das System des Weiteren eine Überkappe (132) beinhaltet, die über dem oberen Ende der Kappe (20, 134) positioniert ist, sodass die Überkappe Kontakt des leitfähigen Körperfluids mit dem ersten und zweiten Material der Teilenergiequelle des Stromsteuerungsgeräts verhindert, bis sich die Überkappe (132) auflöst, wodurch eine Verzögerung zwischen der Zeit des Einbringens des Systems in das Milieu und der Aktivierung des Leitfähigkeitssteuerungsmoduls verursacht und dadurch die Generierung der identifizierbaren Stromsignatur verzögert wird; und/oder wobei das Stromsteuerungsgerät an dem unteren Ende der Kappe befestigt ist, sodass das erste und zweite Material der Teilenergiequelle des Stromsteuerungsgeräts mit dem umgebenden Milieu in Kontakt kommen, nachdem die Kappe von dem Gehäuse ge-
- trennt wird, wodurch das Erzeugen der identifizierbaren Stromsignatur durch das Leitfähigkeitssteuerungsmodul des Stromsteuerungsgeräts verzögert wird.
9. System gemäß einem der vorhergehenden Ansprüche, wobei die Kappe (20, 134) einen sich verjüngenden Abschnitt am unteren Ende umfasst und das Gehäuse (50, 140) einen sich verjüngenden Abschnitt am offenen Ende umfasst, sodass die sich verjüngenden Abschnitte eine Männlich-weiblich-Passung eingehen und zusammengeklebt sind, wodurch verursacht wird, dass die Kappe in dem offenen Ende des Gehäuses befestigt wird, um den Hohlraum abzudichten; und/oder wobei die Kappe mechanisch in das offene Ende des Gehäuses eingepasst wird, um den Hohlraum des Gehäuses abzudichten, und/oder des Weiteren einen pharmazeutischen Wirkstoff beinhaltend, der in dem Hohlraum des Gehäuses (50, 140) positioniert ist und/oder wobei die Vorrichtung eine Zusammensetzung aufweist, die dem Gerät eine Dichte verleiht, die größer als Magenfluid ist.
10. System gemäß einem der vorhergehenden Ansprüche, wobei das System einen Träger beinhaltet, der Folgendes beinhaltet:  
ein lösliches Gehäuse, das einen Hohlraum definiert, wobei das Gehäuse ein offenes Ende und ein geschlossenes Ende umfasst und der pharmazeutische Wirkstoff innerhalb des von dem Gehäuse definierten Hohlraums positionierbar ist.
11. System gemäß Anspruch 10, wobei das Gerät an dem oberen Ende der Kappe befestigt ist, sodass das Gerät mit dem leitfähigen Fluid ungefähr zur gleichen Zeit in Kontakt kommt, zu der das Gehäuse mit dem leitfähigen Fluid in Kontakt kommt.
12. System gemäß einem der Ansprüche 10 bis 11, wobei das Gerät auf dem oberen Ende der Kappe positioniert ist und wobei der Träger des Weiteren eine Überkappe beinhaltet, die um die Kappe herum positioniert und an der Kappe befestigt ist, sodass die Überkappe, indem sie den Kontakt zwischen dem Gerät und dem leitfähigen Fluid verzögert, eine Verzögerung der Aktivierung des Geräts und somit eine Verzögerung der Erzeugung der Stromsignatur verursacht.
13. System gemäß Anspruch 12, wobei das Gerät an einer Unterseite der Überkappe befestigt ist, sodass das Gerät mit dem leitfähigen Fluid in Kontakt kommt, nachdem sich das Gehäuse bis zu dem Punkt aufgelöst hat, an dem die Kappe freigesetzt wird, wodurch eine Verzögerung des Erzeugens der Stromsignatur verursacht wird, und/oder wobei das Gerät innerhalb des von dem Gehäuse definierten

Hohlraums platziert ist, und/oder des Weiteren eine den Auftrieb verändernde Vorrichtung beinhaltend, die innerhalb des von dem Gehäuse definierten Hohlraums positioniert ist.

14. System gemäß einem der vorhergehenden Ansprüche, wobei der Träger des Weiteren eine Füllstoffzusammensetzung beinhaltet, die innerhalb des von dem Gehäuse definierten Hohlraums positioniert ist, um Bewegung des pharmazeutischen Wirkstoffs und des Geräts innerhalb des von dem Gehäuse definierten Hohlraums zu verhindern.

15. System gemäß einem der Ansprüche 12 bis 14, wobei die Überkappe in das offene Ende des Gehäuses (50) geklebt und/oder mechanisch an dem offenen Ende des Gehäuses befestigt und/oder mittels Druck mit dem offenen Ende des Gehäuses verbunden ist.

### Revendications

1. Un système d'administration pharmaceutique pour le suivi de paramètres d'administration, le système comprenant :

un logement de support (50, 140) ayant une extrémité fermée (70) et une extrémité ouverte (60), le logement de support définissant une cavité ;

un agent pharmaceutique pouvant être positionné ou positionné à l'intérieur de la cavité du logement de support ; et

un couvercle (20, 134) comprenant une extrémité de dessus et une extrémité de dessous, l'extrémité de dessous incluant une portion d'étanchéité qui est en communication physique avec l'extrémité ouverte du logement de support afin de fermer de façon étanche la cavité contenant l'agent pharmaceutique, **caractérisé en ce que** le système d'administration pharmaceutique inclut en sus

un dispositif (40, 136) associé au système, le dispositif étant configuré afin de produire une signature de courant identifiable pour la communication d'informations concernant l'administration d'une dose de l'agent pharmaceutique, dans lequel le dispositif est un dispositif de contrôle de courant fixé sur le couvercle et configuré pour la production d'une signature de courant unique, le dispositif de contrôle de courant comprenant :

un module de contrôle de conductance pour la production d'une signature de courant identifiable ; et  
une source d'alimentation partielle compre-

nant un premier matériau et un deuxième matériau isolés l'un par rapport à l'autre et chaque matériau parmi le premier matériau et le deuxième matériau étant couplé électriquement au module de contrôle de conductance, la source d'alimentation partielle du dispositif de contrôle de courant étant configurée afin de produire un potentiel de tension quand le premier matériau et le deuxième matériau sont couplés électriquement par l'intermédiaire d'un fluide conducteur en contact avec ceux-ci et le potentiel de tension étant utilisé afin d'activer le module de contrôle de conductance pour produire la signature de courant identifiable.

2. Le système tel que revendiqué dans la revendication 1, dans lequel la portion d'étanchéité 5 est une portion d'insertion (80).

3. Le système tel que revendiqué dans la revendication 1, dans lequel le dispositif de contrôle de courant est un dispositif formant marqueur d'événement ingérable (IEM, Ingestible Event Marker).

4. Le système de la revendication 1, dans lequel le dispositif est fixé sur l'extrémité de dessus du couvercle de telle sorte que le dispositif puisse entrer en contact avec le milieu environnant lorsque le logement (50, 140) entre en contact avec le milieu environnant.

5. Le système de n'importe lesquelles des revendications précédentes, dans lequel la portion d'étanchéité définit au moins une rainure (92, 94, 96, 98) qui permet au couvercle (20, 134) d'être emboîté par pression dans l'extrémité ouverte (60) du logement de support (50, 140) et/ou dans lequel 20 la portion d'étanchéité est fixée sur l'extrémité ouverte (60) du logement de support à l'aide d'un adhésif et/ou dans lequel la portion d'étanchéité comprend une extrémité compressible, de préférence une extrémité fabriquée à partir d'un matériau compressible, de telle sorte qu'elle puisse être emboîtée par pression dans l'extrémité ouverte (60) du logement de support (50, 140).

6. Le système de n'importe lesquelles des revendications 1 à 5, dans lequel le dispositif est fixé à l'extrémité de dessous de telle sorte que le dispositif entre en contact avec le milieu environnant après que le système a été ingéré et que le couvercle s'est séparé du logement de support.

7. Le système tel que revendiqué dans n'importe lesquelles des revendications précédentes, comprenant :  
un matériau positionné à l'intérieur de la cavité du logement (50, 140) pour la modification de la flotta-

bilité du système.

8. Le système de la revendication 1, dans lequel le dispositif de contrôle de courant est fixé sur l'extrémité de dessus du couvercle de telle sorte que les premier et deuxième matériaux de la source d'alimentation partielle du dispositif de contrôle de courant entrent en contact avec le fluide conducteur 10 environ en même temps que le logement entre en contact avec le fluide conducteur et, par conséquent, le module de contrôle de conductance du dispositif de contrôle de courant est activé lors du contact avec un fluide corporel conducteur ; et/ou dans lequel le dispositif de contrôle de courant (40, 136) est fixé sur l'extrémité de dessus du couvercle (20, 134) et le système comprenant en sus un couvercle coiffant (132) positionné par-dessus l'extrémité de dessus du couvercle (20, 134), de telle sorte que le couvercle coiffant empêche un contact du fluide corporel conducteur avec les premier et deuxième matériaux de la source d'alimentation partielle du dispositif de contrôle de courant jusqu'à ce que le couvercle coiffant (132) se dissolve, ce qui entraîne un retard entre le moment d'introduction du système dans le milieu et l'activation du module de contrôle de conductance et ainsi retarde la génération de la signature de courant identifiable ; et/ou dans lequel le dispositif de contrôle de courant est fixé sur l'extrémité de dessous du couvercle de telle sorte que les premier et deuxième matériaux de la source d'alimentation partielle du dispositif de contrôle de courant entrent en contact avec le milieu environnant après que le couvercle s'est séparé du logement, retardant ainsi la production de la signature de courant identifiable par le module de contrôle de conductance du dispositif de contrôle de courant.
9. Le système tel que revendiqué dans n'importe lesquelles des revendications précédentes, dans lequel le couvercle (20, 134) inclut une portion effilée au niveau de l'extrémité de dessous et le logement (50, 140) inclut une portion effilée au niveau de l'extrémité ouverte de telle sorte que les portions effilées soient un assemblage mâle-femelle et soient collées ensemble, entraînant ainsi la fixation du couvercle dans l'extrémité ouverte du logement afin de fermer de façon étanche la cavité ; et/ou dans lequel le couvercle est emboîté mécaniquement dans l'extrémité ouverte du logement afin de fermer de façon étanche la cavité du logement et/ou comprenant en sus un agent pharmaceutique positionné à l'intérieur de la cavité du logement (50, 140) et/ou dans lequel l'appareil a une composition qui transmet au dispositif une masse volumique qui est supérieure au fluide d'estomac.
10. Le système tel que revendiqué dans n'importe lesquelles des revendications précédentes, le système
- comprenant un support comprenant :  
un logement soluble qui définit une cavité, dans lequel le logement inclut une extrémité ouverte et une extrémité fermée et l'agent pharmaceutique peut être positionné à l'intérieur de la cavité définie par le logement.
11. Le système de la revendication 10, dans lequel le dispositif est fixé sur l'extrémité de dessus du couvercle de telle sorte que le dispositif se mette en contact avec le fluide conducteur environ en même temps que le logement se met en contact avec le fluide conducteur.
12. Le système de n'importe lesquelles des revendications 10 à 11, dans lequel le dispositif est positionné sur l'extrémité de dessus du couvercle et dans lequel le support comprend en sus un couvercle coiffant positionné autour du couvercle et fixé sur le couvercle, de telle sorte que le couvercle coiffant entraîne un retard dans l'activation du dispositif en retardant le contact entre le dispositif et le fluide conducteur et, par conséquent, un retard dans la production de la signature de courant.
13. Le système de la revendication 12, dans lequel le dispositif est fixé sur un dessous du couvercle coiffant de telle sorte que le dispositif entre en contact avec le fluide conducteur après que le logement est dissous jusqu'au point où le couvercle est libéré, entraînant ainsi un retard dans la production de la signature de courant, et/ou dans lequel le dispositif est placé à l'intérieur de la cavité définie par le logement, et/ou comprenant en sus un appareil de modification de flottabilité positionné à l'intérieur de la cavité définie par le logement.
14. Le système tel que revendiqué dans n'importe lesquelles des revendications précédentes, dans lequel le support comprend en sus une composition de remplissage positionnée à l'intérieur de la cavité définie par le logement afin d'empêcher un déplacement de l'agent pharmaceutique et du dispositif à l'intérieur de la cavité définie par le logement.
15. Le système tel que revendiqué dans n'importe lesquelles des revendications 12 à 14, dans lequel le couvercle coiffant est collé dans l'extrémité ouverte du logement (50) et/ou fixé mécaniquement sur l'extrémité ouverte du logement et/ou emboîté par pression dans l'extrémité ouverte du logement.

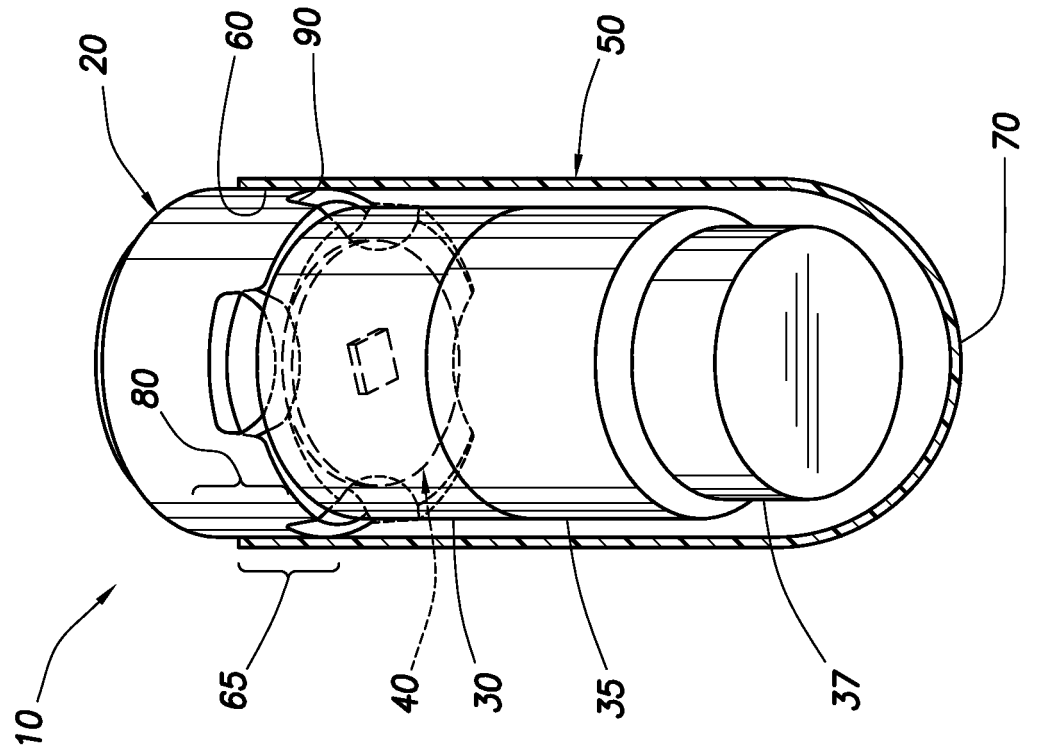


FIG. 1A

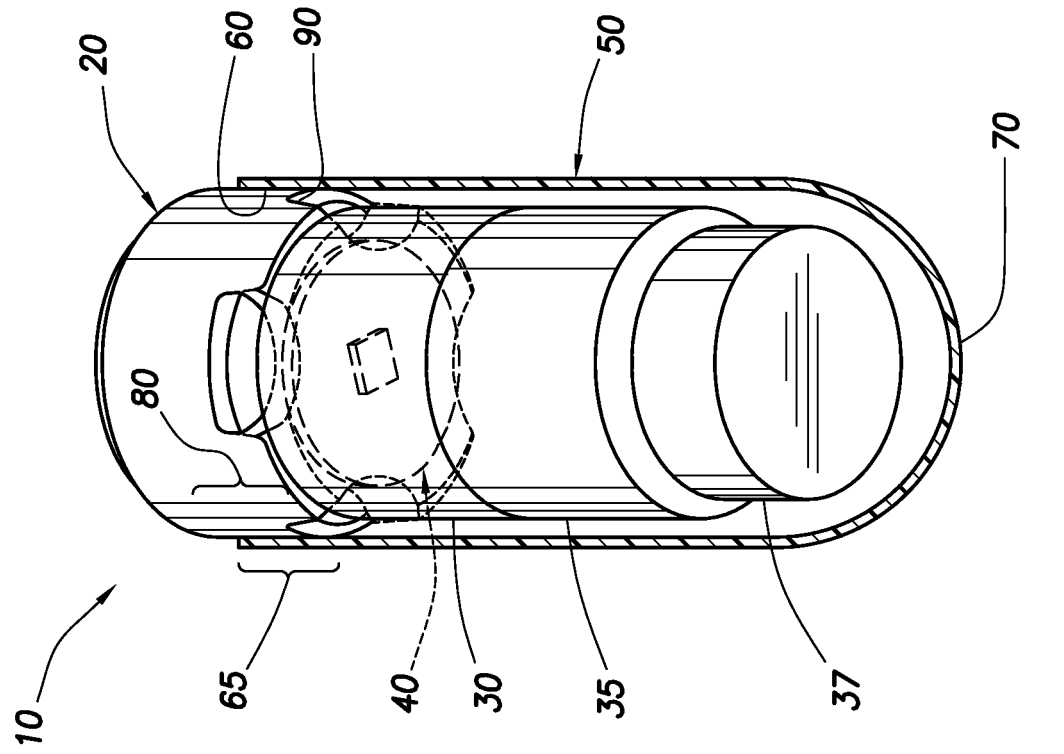


FIG. 1B

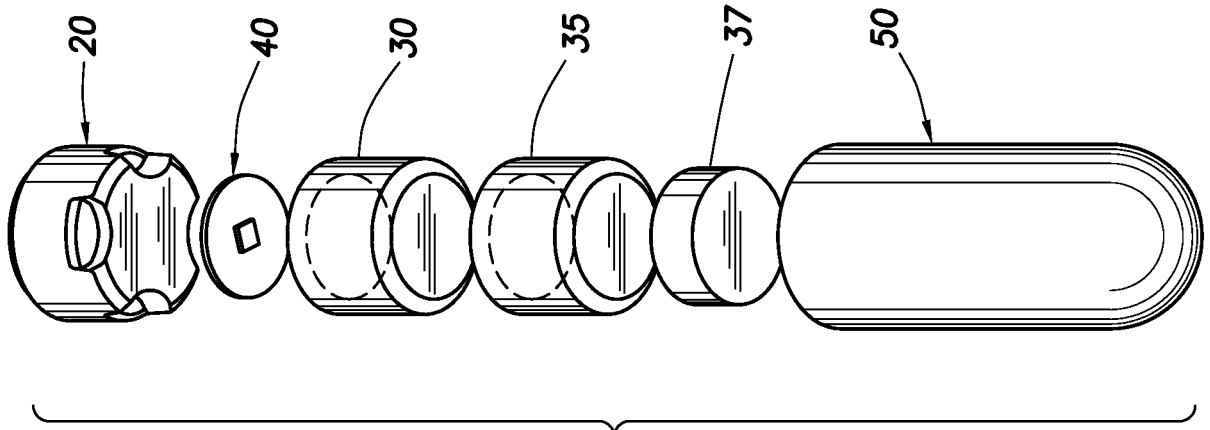


FIG.2B

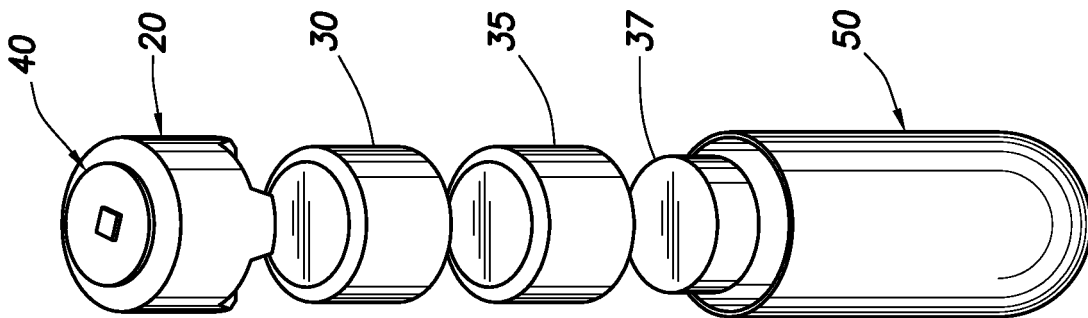
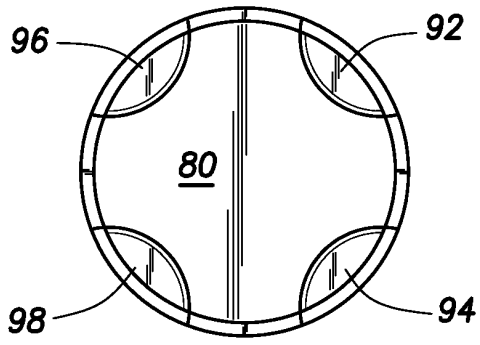
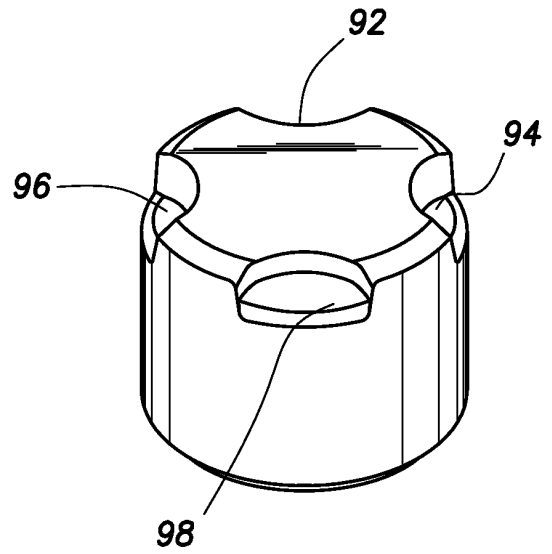


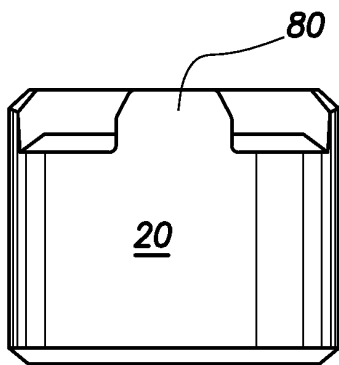
FIG.2A



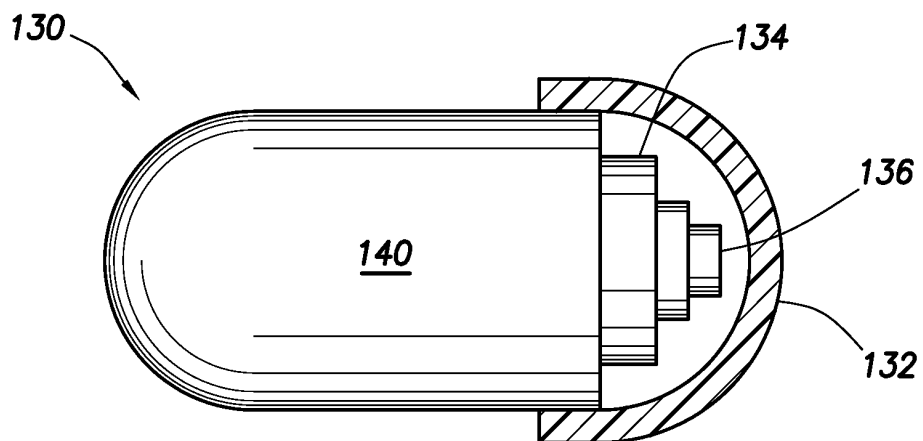
**FIG. 3A**



**FIG. 3C**



**FIG. 3B**



**FIG. 4**

**REFERENCES CITED IN THE DESCRIPTION**

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#### 摘要(译)

根据本发明的用于递送剂量的药物递送系统包括载体组件 ( 50 ) 和帽 ( 20 ), 其配置成密封载体组件的内部体积, 其中帽包括产生独特电流特征的装置 ( 40 ) 。。准备根据本发明的实施方案递送的剂量可用于各种不同的应用, 包括临床试验。