



(11) **EP 2 291 112 B1**

(12) **EUROPEAN PATENT SPECIFICATION**

(45) Date of publication and mention of the grant of the patent:
08.11.2017 Bulletin 2017/45

(21) Application number: **09757912.2**

(22) Date of filing: **20.05.2009**

(51) Int Cl.:
A61B 5/00 (2006.01)

(86) International application number:
PCT/IB2009/052112

(87) International publication number:
WO 2009/147560 (10.12.2009 Gazette 2009/50)

(54) **OPTICAL DETECTION METHOD AND DEVICE FOR OPTICAL DETECTION OF THE CONDITION OF JOINTS**

OPTISCHES NACHWEISVERFAHREN UND GERÄT ZUM OPTISCHEN NACHWEIS DES ZUSTANDS VON GELENKEN

PROCÉDÉ DE DÉTECTION OPTIQUE ET DISPOSITIF DE DÉTECTION OPTIQUE DE L'ÉTAT D'ARTICULATIONS

(84) Designated Contracting States:
AT BE BG CH CY CZ DE DK EE ES FI FR GB GR HR HU IE IS IT LI LT LU LV MC MK MT NL NO PL PT RO SE SI SK TR

(30) Priority: **26.05.2008 EP 08156917**

(43) Date of publication of application:
09.03.2011 Bulletin 2011/10

(73) Proprietor: **Hemics B.V.**
5617 BC Eindhoven (NL)

(72) Inventors:
• **RENSEN, Wouter, H., J.**
NL-5656 AE Eindhoven (NL)

• **VAN BEEK, Michael, C.**
NL-5656 AE Eindhoven (NL)
• **HARBERS, Rik**
NL-5656 AE Eindhoven (NL)

(74) Representative: **Nederlandsch Octrooibureau**
P.O. Box 29720
2502 LS The Hague (NL)

(56) References cited:
WO-A-99/04683 **WO-A-2007/000349**
US-A1- 2001 037 811 **US-B1- 6 222 189**
US-B1- 6 587 704

EP 2 291 112 B1

Note: Within nine months of the publication of the mention of the grant of the European patent in the European Patent Bulletin, any person may give notice to the European Patent Office of opposition to that patent, in accordance with the Implementing Regulations. Notice of opposition shall not be deemed to have been filed until the opposition fee has been paid. (Art. 99(1) European Patent Convention).

Description

FIELD OF INVENTION

[0001] The present invention relates to an optical detection method and to a device for optical detection of the condition of joints.

BACKGROUND OF THE INVENTION

[0002] In the context of the present application, the term light is to be understood to mean non-ionizing electromagnetic radiation, in particular with wavelengths in the range between 400 nm and 1400 nm. The term body part means a part of a human or animal body. The term blocking covers both complete blocking and blocking to a substantial extent.

[0003] In general, the present invention relates to optical detection of joint conditions, in particular to the optical detection of joint diseases such as rheumatoid arthritis (RA). The treatment of such joint diseases is staged. Usually, a patient first receives pain killers. These are frequently followed by non-steroid anti-inflammatory drugs (NSAIDs) and disease modifying anti-rheumatic drugs (DMARDs). In many cases, the last stage in treatment with drugs is the use of biological therapies. In particular the last category is expensive and treatment can cost tens of thousands of dollars per year per patient. Additionally, the drugs used in later stages of treatment often cause more severe side effects. With respect to such joint diseases, medical professionals base their decisions on changes in therapy on disease activity which is given by the number and the severity of inflamed joints.

[0004] Since rheumatoid arthritis is a progressive disease and early diagnosis and start of treatment can help postponing adverse effects and high costs of treatment, there is a demand for methods and devices for providing satisfactory information about the condition of joints and which assist a medical professional to come to a conclusion with respect to the actual joint condition.

[0005] It has been found in time-dependent measurements using non-targeted fluorescent dyes administered to the patient that perfusion dynamics in diseased joints are different as compared to normal healthy joints. However, in the clinical practice of rheumatologists, administration of contrast agents is impractical in most cases.

[0006] As an alternative, it has been proposed to use Diffuse Optical Tomography (DOT) to image joints for providing information about their condition. In a research project, venous blood flow to a body part has been temporarily obstructed by means of a pressure cuff and a single joint has been imaged by means of DOT. In such studies, it has been found that optical parameters exist which correlate with the presence of rheumatoid arthritis (RA).

[0007] For example, it is known that inflammation can be recognized by a change in perfusion. Blood constituents, in particular both oxygenated and deoxygenated

hemoglobin have distinct optical characteristics compared to other constituents of the human or animal body and thus can in principle be optically detected.

[0008] US 6 424 859 B2 discloses a near infrared spectroscopic technique for characterizing the condition of a joint. The results from a spectroscopic measurement are compared to a database in which measurement results for a plurality of arthritic and healthy joints are stored. However, this technique does not allow satisfactorily separating signals resulting from blood and signals from other sources in the body. Further, the technique does not allow separating joint-specific features from features resulting from tissue such as skin, fat, etc. US 6 587 704 B1 discloses a method for non-invasive measurement of blood parameters in which a condition of artificial kinetics by stopping blood flow during measurement. Currently there is no satisfactory tool helping medical professionals in early detection of joint diseases or, more specifically, in quantitative and objective detection of inflamed joints. The same holds for monitoring of disease activity, there is no tool for fast, objective and quantitative detection of disease activity (the degree of inflammation of joints).

SUMMARY OF THE INVENTION

[0009] It is an object of the present invention to provide an optical detection method and a device for optical detection of the condition of joints which provide information about the condition of joints allowing an early detection of joint diseases and allowing monitoring disease activity. The optical detection method and the device for optical detection of the condition of joints shall provide sufficient information to assist a medical professional to come to a conclusion with respect to the joint condition and disease activity, respectively.

[0010] The object is solved by an optical detection method according to claim 1. In the optical detection method, a body part comprising at least one joint is irradiated with light and local attenuation of the light by the body part is detected as attenuation measurements at the position of the at least one joint and at the position of at least one other portion of the body part. Blood flow to and/or from the body part is temporarily at least partially blocked and thereafter enabled again. Distinct local attenuation measurements for the at least one joint and for the at least one other portion of the body part are performed for at least two of the times before, during, and after the blocking of blood flow. Measurements before and after the blocking of the blood flow can give relevant data, if only because it can take the body a remarkable long time (>5 minutes) to fully recover and return to the same transmission properties as before the measurement. Since the attenuation of the light used for irradiation is locally detected for two distinct positions of which at least one is a joint, differences in the optical properties of the at least one joint compared to the at least one other portion of the body part can be detected. Since the distinct local attenuation measurements are performed before

and during the blocking of blood flow, before and after the blocking of blood flow, and/or during and after the blocking of blood flow, the response of the at least one joint to changes in blood flow compared to the at least one other portion can be detected. During inflammation of a joint, the number and properties of blood vessels (capillaries) in the joint change. This effect together with the specific light absorption of blood is used for measuring the condition of a joint. Due to the measurements under different blood flow conditions, the signal resulting from blood can be separated from signals resulting from other sources of light attenuation in the body. Since at least one joint and at least one other body portion of the body part (e.g. next to the joint) are measured, joint-specific results are achieved and contributions from tissues which are present in both the joint and the other body portion (such as fat, skin, etc.) can be separated. As a result, a signal which is joint-specific for changes in blood content can be obtained. Separate measurements to identify the composition (e.g. bone, fat, skin, etc.) of the body part can be omitted. As a consequence, valuable information about the joint condition and/or disease activity is provided to a medical professional. It should be noted that no complete blocking of the blood flow is required but a significant partial reduction in blood flow may suffice.

[0011] Preferably, the distinct local attenuation measurements for the at least one joint and for the at least one other portion of the body part are performed at all three intervals before, during, and after the blocking of blood flow. In this case, even more information about the condition the at least one joint is provided.

[0012] If the at least one other portion of the body part is another joint, the response of different joints to changes in blood flow can be compared and information about differences in the condition of several joints is provided.

[0013] Preferably, for the at least one joint and the at least one other portion of the body part, continuous distinct local attenuation measurements are performed before the blocking of blood flow, during the blocking of blood flow, and after the blocking of blood flow. In this case, due to the continuous measurements, exact information about the time point of a response to a change in blood flow is provided for the at least one joint and the at least one other portion.

[0014] If the results of distinct local attenuation measurements for the at least one joint and for the at least one other portion of the body part which are acquired substantially simultaneously are compared to each other, the differences in response between the at least one joint and the at least one other portion are provided in an advantageous way.

[0015] Preferably, the blood flow is blocked by application of pressure. Thus, a simple and convenient way for obstructing the blood flow is provided.

[0016] According to an aspect, during acquisition of the distinct local attenuation measurements, the body part is immersed in an optically matching medium. In this

case, optical boundary effects and the dynamic range of intensities to which a detector is subjected are reduced.

[0017] The object is further solved by a device for optical detection of the condition of joints according to claim 7. The device comprises: a measurement unit for irradiating a body part comprising at least one joint with light and locally detecting attenuation of the light at the at least one joint and at least one other portion of the body part; a blood flow blocking unit for blocking the blood flow to and/or from the body part; and a control unit. The control unit controls the device such that: blood flow to and/or from the body part is temporarily at least partially blocked and thereafter enabled again; and distinct local attenuation measurements for the at least one joint and for at least one other portion of the body part are performed for at least two of the times before, during, and after the blocking of blood flow. The device achieves the advantages described above with respect to the method.

[0018] If the blood flow blocking unit is adapted to block the blood flow by application of pressure, the advantages can be realized in a simple and convenient way.

[0019] If the measurement unit comprises a light source unit capable of emitting light of at least two distinct wavelengths, one wavelength can be chosen such that blood has a high absorption and another wavelength can be chosen such that the absorption of blood is low or comparable to surrounding tissue. Thus, more detailed information about perfusion of the at least one joint and the at least one other portion of the body part are provided and can be analyzed for judging the condition of the at least one joint.

[0020] Preferably, the light source unit comprises at least two lasers. In this case, well defined wavelengths are provided and differences in perfusion can be detected with high accuracy.

[0021] Preferably, the device is a medical optical detection device.

BRIEF DESCRIPTION OF THE DRAWINGS

[0022] Further features and advantages of the present invention will arise from the detailed description of embodiments with reference to the enclosed drawings.

Fig. 1 schematically shows a set-up for optical detection of the condition of joints according to an embodiment.

Fig. 2 schematically shows details of a measurement unit according to an embodiment.

Fig. 3 schematically shows a human hand as an example for a body part with the positions of joints indicated.

Fig. 4 shows an example for an attenuation measurement as a function of time.

Fig. 5 schematically illustrates the results of simultaneous distinct local attenuation measurements for two joints and one other portion of the body part which is not a joint.

DETAILED DESCRIPTION OF EMBODIMENTS

[0023] An embodiment of the present invention will now be described with reference to the figures. Fig. 1 schematically shows a set-up for the optical detection of the condition of joints. In the illustration, a human body 4 is schematically shown as a body and a hand forms the body part 5 to be examined. However, it should be noted that the invention is not restricted to human bodies and e.g. animal bodies may be subjected to examination. Further, the body part 5 is not restricted to a hand but may also be formed by another body part comprising at least one joint 6 such as arms, legs, feet, etc.

[0024] In the embodiment shown, the device for optical detection of the condition of joints comprises a measurement unit 2, a blood flow blocking unit 3, and a control unit 1. The control unit 1 is provided to control the operation of the device and data acquisition. The measurement unit 2 is provided to irradiate portions of the body part 5 under examination with light and measure the local attenuation of the light at different positions of the body part 5. For example, in the embodiment shown the measurement unit 2 is formed by a measurement head which will be described in more detail below. The blood flow blocking unit 3 is provided for temporarily blocking the blood flow to and/or from the body part 5 under examination. In the embodiment, the blood flow blocking unit 3 is provided by a pressure cuff surrounding the arm to which the hand under examination belongs and obstructing the blood flow by application of pressure to the upper arm. It should be noted that the blood flow blocking unit 3 may be adapted differently in order to allow temporarily at least partially blocking the blood flow to and/or from body parts 5 other than a hand.

[0025] The construction of the measurement unit 2 according to the embodiment will be described in further detail with reference to Fig. 2.

[0026] The measurement unit 2 schematically shown in Fig. 2 is adapted for attenuation measurements in transmission geometry. The measurement unit 2 comprises a light source unit 21 emitting a beam of light for irradiating the body part 5. The light source unit 21 comprises at least one light source and appropriate light guides to direct the beam of light to the body part 5. The light source may be formed by a lamp or by one or more lasers and the light guides may for instance be formed by optical fibers. The light source unit 21 is adapted to be capable to emit light of at least two different wavelengths, preferably in the red to near infrared, wherein one wavelength is chosen such that blood has a high absorption and another wavelength is chosen such that the absorption of blood is low or comparable to surrounding tissue. Suitable wavelengths are for instance 600 nm and 805 nm but other wavelengths fulfilling these criteria are possible as well. Wavelengths in the wavelength range between 550 and 980 nm are particularly suitable. Further, an optical component 22 which e.g. may be formed by a lens is provided for directing the light to the

body part 5. The optical component 22 is capable of concentrating the light (irradiation light 25) on a specific area of interest (or several specific areas of interest; i.e. specific positions) of the body part 5 as will be described below. A second optical element 23 is provided to collect light emerging from the specific area (or areas) of interest and direct the collected light 26 to a detection element 24. The detection element 24 may for instance be formed by a photodiode, a CCD, an optical guide such as a fiber connecting to a photodiode, or another light detection scheme known in the art.

[0027] The measurement unit 2 is adapted such that distinct local attenuation measurements for at least two different portions of the body part 5 can be performed.

[0028] The control unit 1 is adapted such that it controls at least partial blocking of the blood flow to and/or from the body part 5 by means of the blood flow blocking unit 3. Further, it controls the measurement unit 2 such that local attenuation measurements are performed before the blood flow is blocked (interval I in Fig. 4), local attenuation measurements (at the same positions) are performed during the blocking of blood flow (interval II in Fig. 4), and local attenuation measurements (at the same positions) are performed after restoring the blood flow (interval III in Fig. 4).

[0029] Fig. 4 shows an example of attenuation measurements (optical intensity measurements) over time on a finger joint as a particular area of interest before the blocking of blood flow (I), during the blocking of blood flow (II; "occlusion"), and after the blocking of blood flow (III). It can be seen that the attenuation measurements in the three time intervals (before (I), during (II), and after (III) occlusion) are performed continuously to achieve time-resolved measurements. It can be seen that the measured intensity drops after blocking the blood flow and rises again after restoring of the blood flow. However, the height of the drop and the time relation between the blocking/restoring of blood flow and change in the measured intensity provide important information about the condition of the joint 6 under examination.

[0030] According to the invention attenuation measurements are not only performed for a single joint 6 but at least one joint and at least one other portion of the body part under examination are measured simultaneously, i.e. within the same cycle of normal blood flow (I), obstruction of blood flow (II), and restoration of the blood flow (III). This is achieved by simultaneously performing distinct local attenuation measurements at the position of the at least one joint 6 and at the position of the at least one other portion of the body part 5. The at least one other portion of the body part may be another joint or a portion which is not a joint and serves as a reference portion. For each of the positions, attenuation measurements are performed for the at least two different wavelengths of the irradiation light for one of which blood has a high absorption and for the other one of which absorption of blood is low or comparable to surrounding tissue. Preferably, attenuation measurements for multiple joints

of a patient are performed simultaneously. In the preferred embodiment, all joints in both hands are measured simultaneously.

[0031] As a result, the following steps are performed according to the embodiment: distinct local attenuation measurements for at least one joint and at least one other portion of the body part 5 are performed; the blood flow to the body part 5 under examination is temporarily blocked by means of the blood flow blocking unit 3 and distinct local attenuation measurements for the at least one joint and the at least one other portion are performed; and the blood flow is restored and distinct local attenuation measurements for the at least one joint and the at least one other portion of the body part 5 are performed. In each of the intervals, several attenuation measurements are performed to achieve a time-resolved measurement. Further, the time dependent behavior of the at least one joint and the at least one other portion of the body part 5 are analyzed both independently and with respect to each other. Exploiting the measurements for at least two different wavelengths allows analyzing the perfusion dynamics and oxygenation.

[0032] Preferably, multiple joints are measured simultaneously and the time dependent behavior of these multiple joints with respect to each other is analyzed. Still more preferably, all joints of a body part 5 are measured simultaneously. Fig. 3 shows a hand as an example for a body part 5 to be examined and the positions of joints 6 are indicated by crosshairs (it should be noted that not all joints are provided with reference signs). The indicated positions can be used as positions for the local attenuation measurements and additionally positions between these indicated positions can be used for reference attenuation measurements.

[0033] In the embodiment shown in Fig. 1, via the measurement unit 2, the control unit 1 detects the spectral characteristics of the body part 5 containing joints 6. After a baseline measurement, the blood flow is (at least partially) blocked by the blood flow blocking unit 3. The measurement unit 2 now detects spectral changes related to the reduced blood flow. After some time, e.g. 30 seconds, the blood flow is restored by operating the blood flow blocking unit 3 appropriately (e.g. releasing the pressure cuff). The measurement unit 2 detects how fast the perfusion is restored in the joints and in which order the perfusion is restored. Preferably, the perfusion recovery is also compared between joints and other areas of the body part 5. Inflamed joints will have a different perfusion and oxygenation as compared to healthy joints. As a result, the dynamic spectral behavior which is measured by the measurement unit 2 will be different.

[0034] Fig. 5 shows an example for the results of attenuation measurements (in transmission geometry) performed simultaneously. The trace marked with T1 corresponds to local attenuation measurements at a first joint, the trace marked with T2 corresponds to local attenuation measurements at a second joint, and the trace marked with R1 corresponds to local attenuation measurements

at a reference position which is not a joint. The characteristics A, B, C of the drops occurring in the traces can be different. Thus, a single drop can be analyzed and also the relation between the drops A, B, C in the different traces T1, T2, and R1. Inflamed joints can show signs of high perfusion such as an increased drop in transmission compared to other joints or compared to a reference position. Also the time differences D, E between the changes in transmission between the traces T1, T2, and R1 can be used as marker for inflammation and provide important information.

[0035] The time-dependent behavior of individual joints, the behavior of joints with respect to each other and with respect to other parts (that can act as a reference) is analyzed.

[0036] In the embodiment described above, the measurement unit 2 has been adapted for measurements in transmission geometry, i.e. the body part is irradiated from one side and the light having passed through the body part is measured on the opposite side. In a modification of the embodiment, the measurement unit 2 can be adapted for attenuation measurements in reflection geometry. In this case, irradiation and detection are performed from the same side of the body part 5. In reflection geometry, the optical components 22 and 23 can be combined. It is advantageous to separate the diffuse reflected light from the illumination light. This can be achieved e.g. by orthogonal polarized spectral imaging (OPSI) or dark-field imaging or other suitable techniques known in the art.

[0037] It should be noted that, in the embodiments, the blood flow need not be completely blocked but a substantial reduction of the blood flow may suffice.

[0038] A plurality of different ways for implementing the measurement unit 2 exists. It is an essential feature that the local collection of light from multiple portions of the body part 5 under examination is measured. This can e.g. be achieved by illuminating a single spot at a time and detecting a corresponding single spot on the body part 5 and scanning the position of the illumination and detection spot over the body part 5.

[0039] A further, more preferred possibility is to illuminate the whole body part 5 and to image the transmitted (or reflected) light with a CCD camera or another suitable camera. However, due to the diffuse transmission, in this case the resolution of the image is limited and light traveling e.g. between fingers may overload the detector.

[0040] A still more preferred possibility is to illuminate a discrete number of spots on the body part 5. This implementation has the advantage that less stray light reaches the detector which leads to a higher resolution and that the intensity of all the spots can be adjusted such that only a limited dynamic range is required for the detector.

[0041] It is also possible to immerse the body part 5 under examination in an optically matching medium, e.g. a fluid, in order to reduce optical boundary effects and the dynamic range of intensities falling on the detector.

In such a technique, a fluid having optical properties (such as the optical absorption coefficient and the reduced scattering coefficient) similar to those of tissue is employed.

[0042] Further, to detect different wavelengths, it is possible to alternate the illumination wavelength. It is also possible to illuminate with all required wavelengths simultaneously and separate the different wavelengths in the detection path, e.g. using filters or a spectrograph.

[0043] In a preferred implementation, multiple body parts (e.g. both hands) are measured simultaneously.

[0044] Although it has been described with respect to the embodiment that at least two wavelengths are used for illumination, the invention is not restricted to that. For example, a larger number of discrete wavelengths can be used or even a complete spectrum over a certain range of wavelengths (e.g. 650 to 1000 nm). However, acquiring a complete spectrum requires more costly components as compared to a few distinct wavelengths. If several types of tissue components (such as fat, water, etc.) shall be discriminated, it might be advantageous to use more than two distinct wavelengths. Using more wavelengths helps improving the accuracy of the device, however, at increased cost and complexity.

Claims

1. Optical detection method of the condition of joints; wherein a body part (5) comprising at least one joint (6) is irradiated with light; and local attenuation of the light by the body part (5) is substantially simultaneously detected as attenuation measurement at the position of the at least one joint (6) and at the position of at least one other portion of the body part (5); and wherein blood flow to and/or from the body part (5) is temporarily at least partially blocked and thereafter enabled again; distinct local attenuation measurements for the at least one joint (6) and for at least one other portion of the body part (5) are substantially simultaneously performed for at least two of the times before (I), during (II), and after (III) the blocking of blood flow; and wherein the results of the distinct local attenuation measurements for the at least one joint (6) and for the at least one other portion of the body part (5) are compared to each other.
2. Optical detection method according to claim 1, wherein the distinct local attenuation measurements for the at least one joint (6) and for the at least one other portion of the body part are performed before (I), during (II), and after (III) the blocking of blood flow.
3. Optical detection method according to any one of claims 1 and 2, wherein the at least one other portion of the body part (5) is another joint.
4. Optical detection method according to any one of claims 1 to 3, wherein, for the at least one joint (6) and the at least one other portion of the body part (5), continuous distinct local attenuation measurements are performed before the blocking of blood flow (I), during the blocking of blood flow (II), and after the blocking of blood flow (III).
5. Optical detection method according to any one of claims 1 to 4, wherein the blood flow is blocked by application of pressure.
6. Optical detection method according to any one of claims 1 to 5, wherein, during acquisition of the distinct local attenuation measurements, the body part (5) is immersed in an optically matching medium.
7. Device for optical detection of the condition of joints; the device comprising:
 - a measurement unit (2) for irradiating a body part (5) comprising at least one joint (6) with light and locally and substantially simultaneously detecting attenuation of the light at the at least one joint (6) and at least one other portion of the body part (5);
 - a blood flow blocking unit (3) for blocking the blood flow to and/or from the body part (5);
 - and a control unit (1) controlling the device such that:
 - blood flow to and/or from the body part (5) is temporarily at least partially blocked and thereafter enabled again; and
 - distinct local attenuation measurements for the at least one joint (6) and for at least one other portion of the body part (5) are substantially simultaneously performed for at least two of the times before (I), during (II), and after (III) the blocking of blood flow, and the results of the distinct local attenuation measurements for the at least one joint (6) and for the at least one other portion of the body part (5) are compared to each other.
8. Device for optical detection of the condition of joints according to claim 7, wherein the blood flow blocking unit (3) is adapted to block the blood flow by application of pressure.
9. Device for optical detection of the condition of joints according to any one of claims 7 and 8, wherein the measurement unit (2) comprises a light source unit (21) capable of emitting light of at least two distinct wavelengths.

10. Device for optical detection of the condition of joints according to claim 9, wherein the light source unit (21) comprises at least two lasers.

Patentansprüche

1. Verfahren zur optischen Detektion des Zustands von Gelenken, wobei ein Körperteil (5), das wenigstens ein Gelenk (6) enthält, mit Licht bestrahlt wird und lokale Abschwächung des Lichts durch das Körperteil (5) im Wesentlichen gleichzeitig als Abschwächungsmessung an der Position des wenigstens einen Gelenks (6) und an der Position von wenigstens einem anderen Bereich des Körperteils (5) detektiert wird, und wobei der Blutfluss zu und/oder von dem Körperteil (5) zeitweilig wenigstens teilweise blockiert und danach wieder freigegeben wird, verschiedene lokale Abschwächungsmessungen für das wenigstens eine Gelenk (6) und für wenigstens einen anderen Bereich des Körperteils (5) im Wesentlichen gleichzeitig zu wenigstens zwei Zeitpunkten von vor (I), während (II) und nach (III) der Blockierung des Blutflusses durchgeführt werden und wobei die Resultate der verschiedenen lokalen Abschwächungsmessungen für das wenigstens eine Gelenk (6) und für den wenigstens einen anderen Bereich des Körperteils (5) miteinander verglichen werden.
2. Verfahren zur optischen Detektion nach Anspruch 1, wobei die verschiedenen lokalen Abschwächungsmessungen für das wenigstens eine Gelenk (6) und für den wenigstens einen anderen Bereich des Körperteils durchgeführt werden vor (I), während (II) und nach (III) der Blockierung des Blutflusses.
3. Verfahren zur optischen Detektion gemäß einem der Ansprüche 1 und 2, wobei der wenigstens eine andere Bereich des Körperteils (5) ein anderes Gelenk ist.
4. Verfahren zur optischen Detektion nach einem der Ansprüche 1 bis 3, wobei, für das wenigstens eine Gelenk (6) und den wenigstens einen anderen Bereich des Körperteils (5), verschiedene lokale Abschwächungsmessungen kontinuierlich durchgeführt werden vor der Blockierung des Blutflusses (I), während der Blockierung des Blutflusses (II) und nach der Blockierung des Blutflusses (III).
5. Verfahren zur optischen Detektion nach einem der Ansprüche 1 bis 4, wobei der Blutfluss durch Anwenden von Druck blockiert wird.

6. Verfahren zur optischen Detektion nach einem der Ansprüche 1 bis 5, wobei, während der Aufnahme der verschiedenen lokalen Abschwächungsmessungen, das Körperteil (5) in ein optisches Anpassungsmedium eingetaucht ist.

7. Gerät für die optische Detektion des Zustands von Gelenken, wobei das Gerät aufweist:
- eine Messeinheit (2) zum Bestrahlen eines Körperteils (5), das wenigstens ein Gelenk (6) enthält, mit Licht und zum im Wesentlichen gleichzeitigen Detektieren der Lichtabschwächung an dem wenigstens einen Gelenk (6) und an wenigstens einem anderen Bereich des Körperteils (5),
- eine Blutfluss-Blockiereinheit (3) zum Blockieren des Blutflusses zu und/oder von dem Körperteil (5)
- und eine Steuereinheit (1), die das Gerät so steuert, dass:

der Blutfluss zu und/oder von dem Körperteil (5) zeitweilig wenigstens teilweise blockiert und danach wieder freigegeben wird und verschiedene lokale Abschwächungsmessungen für das wenigstens eine Gelenk (6) und für den wenigstens einen anderen Bereich des Körperteils (5) im Wesentlichen simultan durchgeführt werden zu wenigstens zwei Zeitpunkten von vor (I), während (II) und nach (III) der Blockierung des Blutflusses und die Resultate der verschiedenen lokalen Abschwächungsmessungen für das wenigstens eine Gelenk (6) und für den wenigstens einen anderen Bereich des Körperteils (5) miteinander verglichen werden.

8. Gerät zur optischen Detektion des Zustands von Gelenken nach Anspruch 7, wobei die Blutfluss-Blockiereinheit (3) dazu ausgestaltet ist, den Blutfluss durch Anwendung von Druck zu blockieren.
9. Gerät zur optischen Detektion des Zustands von Gelenken nach einem der Ansprüche 7 und 8, wobei die Messeinheit (2) eine Lichtquelleneinheit (21) aufweist, die zur Ausstrahlung von Licht mit wenigstens zwei verschiedenen Wellenlängen in der Lage ist.
10. Gerät zur optischen Detektion des Zustands von Gelenken nach Anspruch 9, wobei die Lichtquelleneinheit (21) wenigstens zwei Laser aufweist.

Revendications

1. Méthode de détection optique de l'état d'articulations ; dans laquelle une partie de corps (5) comprenant au moins une articulation (6) est irradiée à l'aide d'une lumière ; et une atténuation locale de la lumière par la partie de corps (5) est détectée de manière sensiblement simultanée comme une mesure d'atténuation à la position de la au moins une articulation (6) et à la position d'au moins une autre partie de la partie de corps (5) ; et dans laquelle un écoulement sanguin vers et/ou depuis la partie de corps (5) est temporairement au moins partiellement bloqué et après ceci autorisé à nouveau ; des mesures d'atténuation locale distinctes pour la au moins une articulation (6) et pour la au moins une autre partie de la partie de corps (5) sont effectuées de manière sensiblement simultanée pour au moins deux instants parmi avant (I), pendant (II), et après (III) le blocage de l'écoulement sanguin ; et dans laquelle les résultats des mesures d'atténuation locale distinctes pour la au moins une articulation (6) et pour la au moins une autre partie de la partie de corps (5) sont comparés l'un à l'autre.
2. Méthode de détection optique selon la revendication 1, dans laquelle les mesures d'atténuation locale distinctes pour la au moins une articulation (6) et pour la au moins une autre partie de la partie de corps sont effectuées avant (I), pendant (II), et après (III) le blocage de l'écoulement sanguin.
3. Méthode de détection optique selon l'une quelconque des revendications 1 et 2, dans laquelle la au moins une autre partie de la partie de corps (5) est une autre articulation.
4. Méthode de détection optique selon l'une quelconque des revendications 1 à 3, dans laquelle, pour là au moins une articulation (6) et la au moins une autre partie de la partie de corps (5), des mesures d'atténuation locale distinctes continues sont effectuées avant le blocage de l'écoulement sanguin (I), pendant le blocage de l'écoulement sanguin (II), et après le blocage de l'écoulement sanguin (III).
5. Méthode de détection optique selon l'une quelconque des revendications 1 à 4, dans laquelle l'écoulement sanguin est bloqué par application d'une pression.
6. Méthode de détection optique selon l'une quelconque des revendications 1 à 5, dans laquelle, pendant l'acquisition des mesures d'atténuation locale distinctes, la partie de corps (5) est immergée dans un milieu optiquement correspondant.
7. Dispositif de détection optique de l'état d'articulations ; le dispositif comprenant :
 - une unité de mesure (2) pour irradier une partie de corps (5) comprenant au moins une articulation (6) à l'aide d'une lumière et détecter localement et de manière sensiblement simultanée une atténuation de la lumière au niveau de la au moins une articulation (6) et d'au moins une autre partie de la partie de corps (5) ;
 - une unité de blocage d'écoulement sanguin (3) pour bloquer l'écoulement sanguin vers et/ou depuis la partie de corps (5) ;
 - et une unité de commande (1) commandant le dispositif de telle sorte que :
 - l'écoulement sanguin vers et/ou depuis la partie de corps (5) est temporairement au moins partiellement bloqué et après ceci autorisé à nouveau ; et des mesures d'atténuation locale distinctes pour la au moins une articulation (6) et pour la au moins une autre partie de la partie de corps (5) sont effectuées de manière sensiblement simultanée pour au moins deux instants parmi avant (I), pendant (II), et après (III) le blocage de l'écoulement sanguin, et les résultats des mesures d'atténuation locale distinctes pour la au moins une articulation (6) et la au moins une autre partie de la partie de corps (5) sont comparés l'un à l'autre.
8. Dispositif de détection optique de l'état d'articulations selon la revendication 7, dans lequel l'unité de blocage d'écoulement sanguin (3) est adaptée pour bloquer l'écoulement sanguin par application d'une pression.
9. Dispositif de détection optique de l'état d'articulations selon l'une quelconque des revendications 7 et 8, dans lequel l'unité de mesure (2) comprend une unité de source lumineuse (21) capable d'émettre une lumière ayant au moins deux longueurs d'onde distinctes.
10. Dispositif de détection optique de l'état d'articulations selon la revendication 9, dans lequel l'unité de source lumineuse (21) comprend au moins deux lasers.

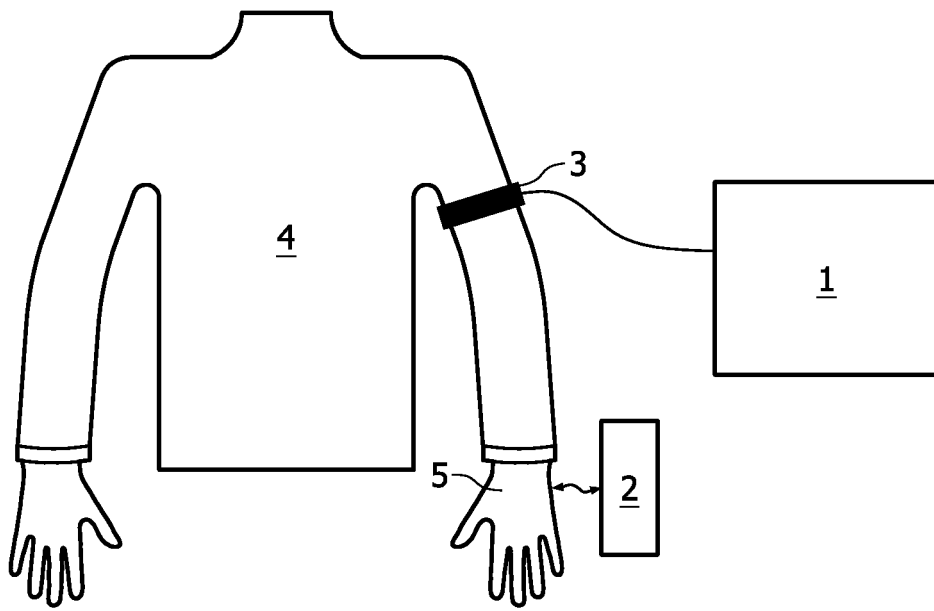


FIG. 1

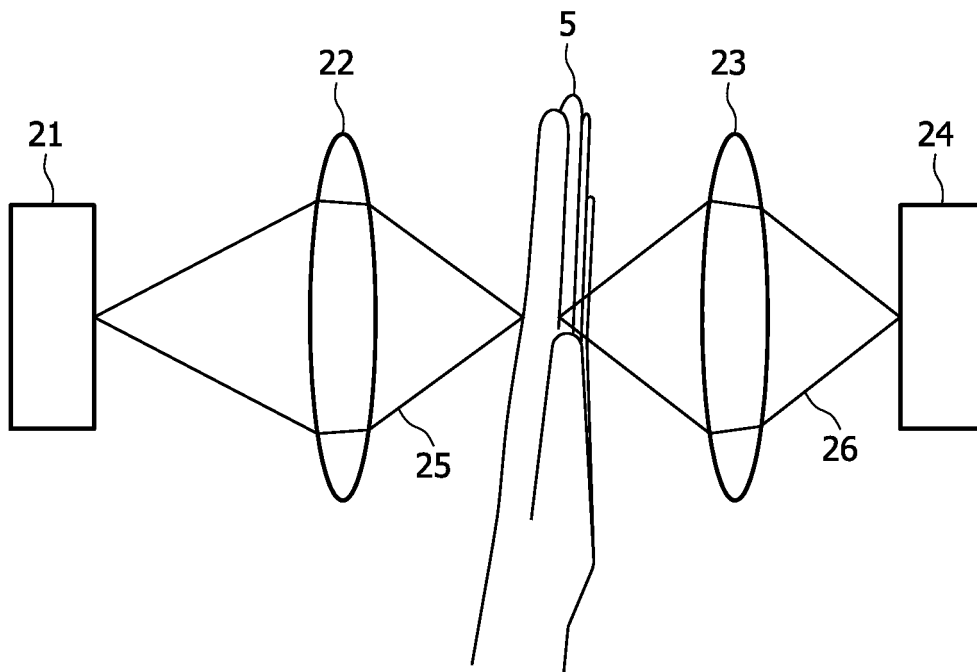


FIG. 2

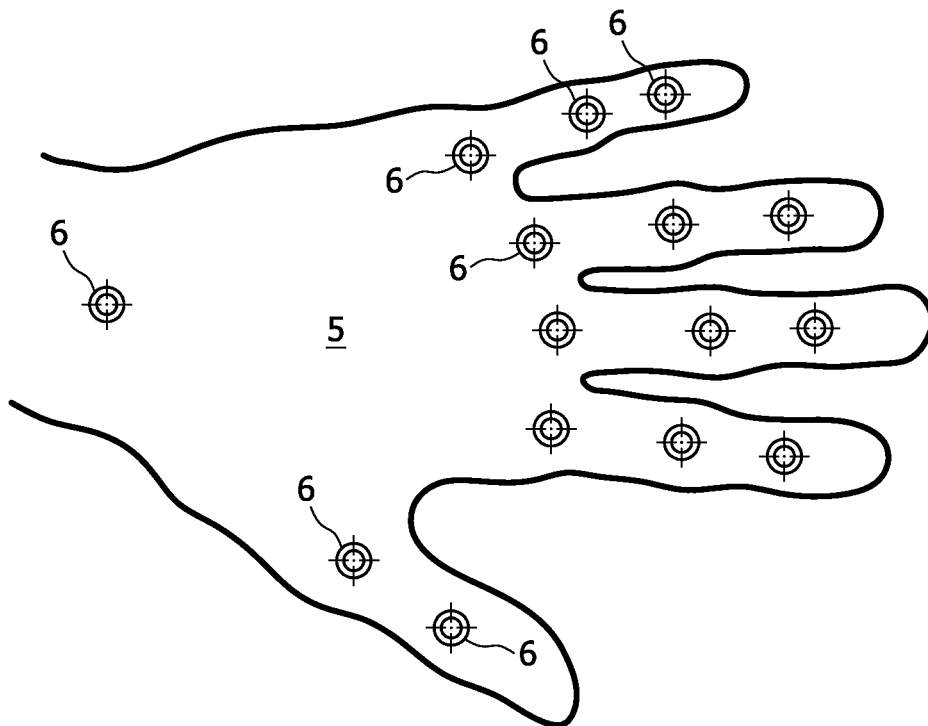


FIG. 3

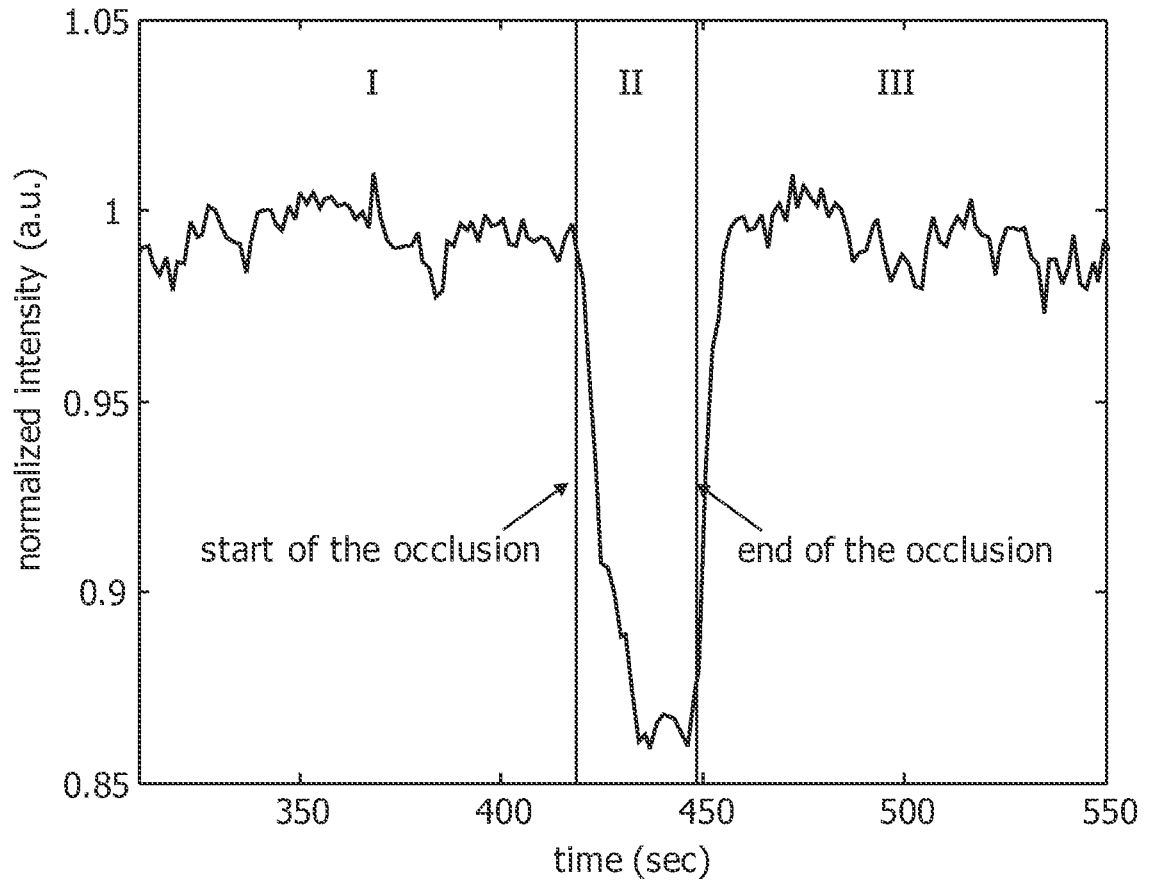


FIG. 4

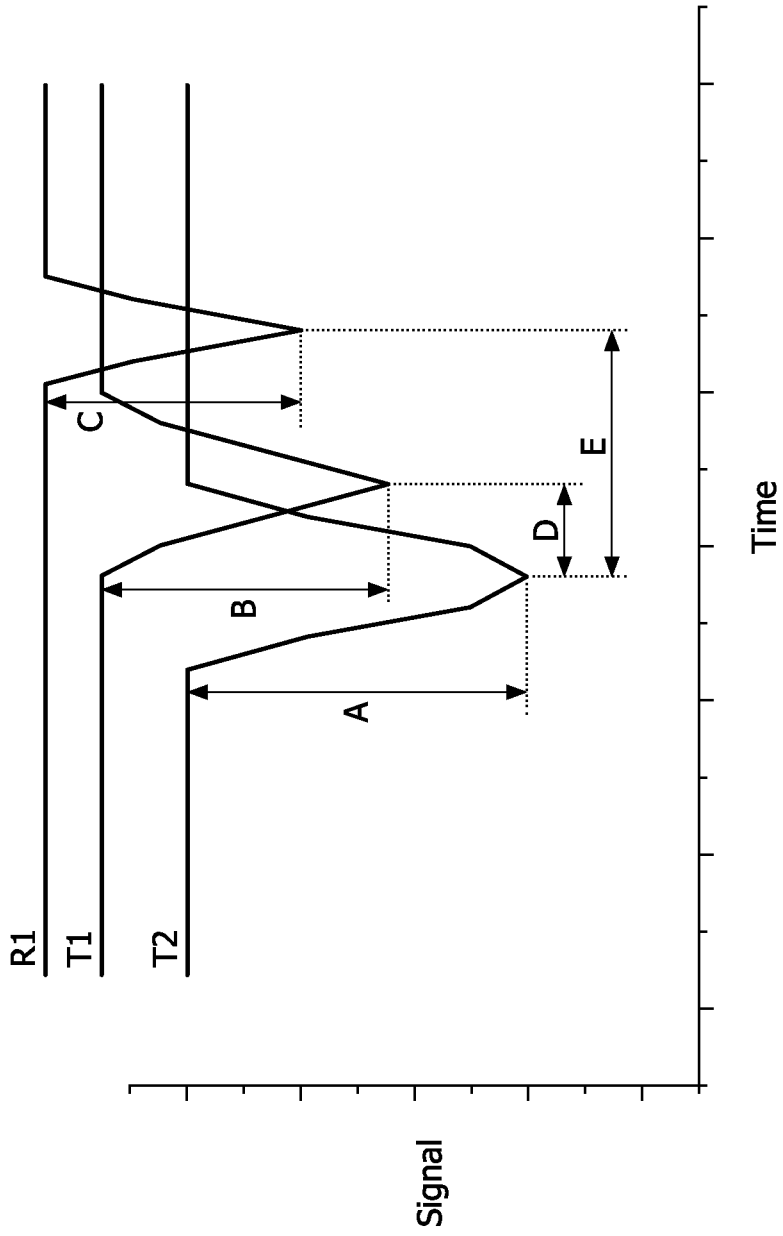


FIG. 5

REFERENCES CITED IN THE DESCRIPTION

This list of references cited by the applicant is for the reader's convenience only. It does not form part of the European patent document. Even though great care has been taken in compiling the references, errors or omissions cannot be excluded and the EPO disclaims all liability in this regard.

Patent documents cited in the description

- US 6424859 B2 [0008]
- US 6587704 B1 [0008]

| | | | |
|----------------|------------------------------------------------------------------|---------|------------|
| 专利名称(译) | 用于光学检测关节状态的光学检测方法和装置 | | |
| 公开(公告)号 | EP2291112B1 | 公开(公告)日 | 2017-11-08 |
| 申请号 | EP2009757912 | 申请日 | 2009-05-20 |
| [标]申请(专利权)人(译) | 皇家飞利浦电子股份有限公司 | | |
| 申请(专利权)人(译) | 皇家飞利浦电子N.V. | | |
| 当前申请(专利权)人(译) | HEMICS B.V. | | |
| [标]发明人 | RENSSEN WOUTER H J VAN BEEK MICHAEL C HARBERS RIK | | |
| 发明人 | RENSSEN, WOUTER, H., J. VAN BEEK, MICHAEL, C. HARBERS, RIK | | |
| IPC分类号 | A61B5/00 | | |
| CPC分类号 | A61B5/0059 A61B5/02007 A61B5/4528 A61B5/6826 A61B5/6838 | | |
| 代理机构(译) | NEDERLANDSCH OCTROOIBUREAU | | |
| 优先权 | 2008156917 2008-05-26 EP | | |
| 其他公开文献 | EP2291112A2 | | |
| 外部链接 | Espacenet | | |

摘要(译)

提供一种光学检测方法，其中用光照射包括至少一个接头（6）的主体部分（5）。由身体部分（5）对光的局部衰减被检测为在至少一个关节（6）的位置处和在身体部分（5）的至少一个其他部分的位置处的衰减测量值；并且其中流入和/或来自身体部分（5）的血液暂时至少部分地被阻塞，然后再次启用。对于至少一个关节（6）和身体部位（5）的至少一个其他部分的不同的局部衰减测量在（I），（II）和之后（III）中的至少两个时间执行。) 阻断血液流动。

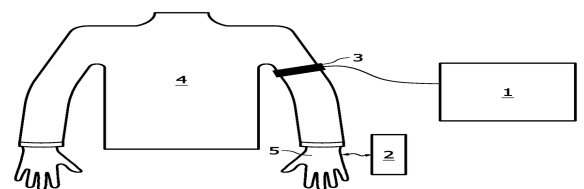


FIG. 1

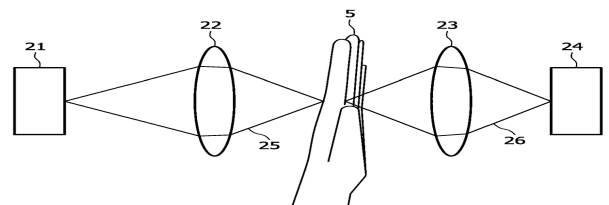


FIG. 2