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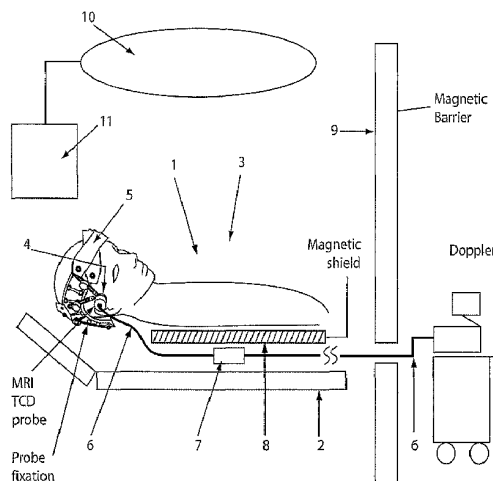
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(54) Title: **ULTRASOUND IN MAGNETIC SPATIAL IMAGING APPARATUS**



(57) Abstract: The present invention provides apparatus and methods for acquiring ultrasound measurements representing biosignals from a subject located in the strong magnetic field of a spatial imaging device. The invention includes ultrasound probes having minimal magnetic parts and an ultrasound signal pre-amplifier being shielded by a barrier or barriers from the strong magnetic field of a spatial imaging device such as an MRI, PET, or CT scanner. Most preferably, the ultrasound probe produces ultrasound waves in the frequency range of approximately 2.0 MHz to 2.5 MHz. The ultrasound probe may include no electronic components and contains minimal magnetic or ferromagnetic parts. The elements for acquiring and analysing ultrasound waves may be located in separate rooms from the imaging device. The invention provides a method of taking ultrasound measurements in quick succession with measurements of a spatial imaging device to provide a more informative understanding of the physiology of the subject.

Ultrasound in Magnetic Spatial Imaging Apparatus

5 **Field of the Invention**

This invention relates to methods and apparatus for measuring physiological parameters, in particular blood flow rates and electrophysiological activity, using ultrasound and spatial imaging techniques.

10

Background

Developments in imaging techniques have made it possible to measure physiological parameters over differing timeframes by exploiting the physics of waveforms as they pass through heterogeneous tissues. For example, it is known in the art that the properties of the diffraction of sound waves of very high frequency (known as the Doppler effect) directed toward moving fluids, including blood moving through vessels, can be analysed to measure blood flow-rate. Such techniques using sound waves (known as ultrasound technologies) have been conveniently used in applications of cardiology and, more recently, brain blood-flow. Further developments in the use of ultrasound in brain blood-flow measurements are known in the art where measurements are made using ultrasound penetrating the cranium (Transcranial Doppler, or TCD). Such techniques were disclosed by Aaslid in US patent no. 4,817,621, which described apparatus for TCD to measure blood-flow in vessels in the brain.

25 Other developments for making images of tissue *in situ* have occurred independently, using different principles of physics, such as measuring concentrations of particular atoms and molecules with varying concentrations in heterogeneous tissues by activating the atoms and molecules by strong magnetic fields and measuring the activation. Such a technique is known in the art of magnetic resonance imaging (MRI).

30

Both ultrasound and MRI are used to measure aspects of fluids in tissues. However, the techniques, like other imaging techniques, operate on different timescales and can be interpreted for different physiological parameters. The speed with which ultrasound waves can be generated, reflected and analysed is over periods of milliseconds. The speed at which MRI

images can be generated is at least tenfold slower. Ultrasound measurements show immediate and dynamically changing flow rates of fluids such as blood. Ultrasound measurements inform little about anatomy or morphology of the tissues being penetrated. MRI measurements are static but very rich in anatomical and morphological information.

5

A great advantage would occur if physiological information could be derived from both ultrasound and MRI measurements of a tissue. This would be particularly advantageous for TCD blood-flow measurements of brain tissue made concurrently with MRI structural measurements. A device and method for concurrently taking ultrasound and MRI
10 measurements, or at least in quick succession, of the same tissue could collectively provide much more information than independent, non-concurrent measurements made using either technique.

While making concurrent or quick successive measurements of physiological parameters using
15 ultrasound and other imaging techniques like MRI would be advantageous, it has not been possible to date. A major reason is because the strong magnetic fields of MRI induce currents in electrical conducting materials. Such conducting materials are commonly used in ultrasound devices. The currents interfere with, and make it impossible to generate and receive, ultrasound waves for analysis. What is needed is ultrasound apparatus, in particular TCD
20 apparatus, that is unaffected, or minimally affected by the magnetic fields of imaging systems such as MRI systems, to enable the concurrent or quick successive measurements of physiological parameters to enable independent and dynamic measurements of physiological processes. Similarly, methods for concurrently or quick successive measuring physiological parameters with ultrasound and MRI are needed. Such methods and apparatus would have
25 many applications such as measuring blood flow during disease events such as stroke which is associated with abnormal blood flows in the brain.

Summary of the Invention

It is known in the art that ultrasound transducer probes for generating, transmitting and receiving
30 ultrasound waves are comprised of magnetic materials including a coil for amplifying the reflected ultrasound signal received by the probe. Conventionally within the member is a crystal that vibrates to produce the ultrasound waves, the crystal being adjacent or nearly adjacent the amplifying coil needed to amplify signals for processing. However, placing such a probe within the magnetic field of magnetic imaging system such as an MRI scanner results in the induction

of electrical currents in the coils by the magnetic field of the imaging system, the result being that the ultrasound probe is unusable for generating and receiving meaningful ultrasound signals. Surprisingly, the invention provides that the received ultrasound signal amplifier can be spatially separated from the ultrasound-generating crystal, outside the strong magnetic field of the imaging system, but in electrical communication with a suitable conducting connector so that the received ultrasound signal may be amplified and further processed outside the magnetic field. The result is that ultrasound signals representative of physiological processes can be measured in quick succession with the operation of the magnetic imaging system, notwithstanding the presence of the ultrasound member within the magnetic field of the magnetic imaging system.

The invention most advantageously provides apparatus and methods for measuring both ultrasound signals and magnetic imaging modalities. In one aspect the invention most advantageously provides a method of making at least one ultrasound imaging measurement using ultrasound apparatus within the magnetic field of a spatial imaging device having a magnetic field successively with making magnetic spatial images with the spatial imaging device, the method including the steps of:

- a. positioning at least one non-magnetic ultrasound member adjacent a subject for making an ultrasound measurement;
- b. establishing electrical communication with the at least one non-magnetic ultrasound member with an ultrasound signal pre-amplifier;
- c. magnetically isolating the magnetic field of the spatial-image device from said signal pre-amplifying means;
- d. operating the at least one ultrasound member and an ultrasound imaging means to create a physiological signal of fluid flow in the subject;
- e. interrupting the operation of the ultrasound member and ultrasound imaging means;
- f. operating the spatial imaging device to record an image during said interruption; and
- g. repeating steps e and f, if desired.

In another aspect, the invention provides apparatus for making ultrasound measurements of fluid flow in a subject located in a spatial imaging device having a strong magnetic field, including: a least one ultrasound member for generating ultrasound waves, said member having minimal magnetic parts; electrical signal communication means in communication with the at least one ultrasound member; electrical signal amplifying means; magnetic field barrier for

magnetically shielding the signal amplifying means; and an imaging device having a strong magnetic field wherein said magnetic field barrier is disposed to shield said signal amplifying means from said magnetic field of said imaging device. Preferably wherein the ultrasound member is an ultrasound probe for producing ultrasound waves in the frequency range of approximately 1 MHz to 4 MHz. More preferably, the ultrasound probe for produce ultrasound waves in the frequency range of approximately 2.0 MHz to 2.5 MHz. Preferably, the ultrasound member includes no electronic components. Preferably, the apparatus contains minimal magnetic or ferromagnetic parts in the ultrasound member. The ultrasound member may include conducting parts comprised of carbon materials. Other embodiments include parts in the ultrasound member being comprised of substances that minimise artefacts or distortion to the image modality image and analysis processing. The elements for acquiring and analysing ultrasound waves may be located in separate rooms from the imaging device wherein the magnetic field barrier is the wall of an enclosure. Preferably, the apparatus includes a headband for positioning at least one ultrasound member for taking ultrasound measurements. Preferably, the headband is comprised of a non-magnetic material or materials. Preferably the spatial imaging device is any one of an MRI scanner, PET scanner, or CT scanner.

Brief Description of the Figures

Figure 1 shows a diagram of the features of the invention.

Figure 2 shows an embodiment of non-magnetic ultrasound members for use in magnetic fields.

Figure 3 shows a side view of a non-magnetic ultrasound member held in place with a non-magnetic band for use in magnetic fields.

Figure 4 shows a front view of two non-magnetic ultrasound members held in place with a non-magnetic band for use in magnetic fields.

Detailed Description of the Figures and Most Preferred Embodiments

The invention is most easily understood with reference to the accompanying figures. Figure 1 shows an embodiment of the invention, including the elements necessary to acquire ultrasound signals and spatial imaging information using strong magnetic fields. It will be understood that other embodiments of the invention are possible and that the scope of the invention is not limited to the embodiments described herein. In Figure 1 is shown a subject 1 in a prone position on a table 2 within the magnetic field 3 of a spatial imaging device 10. The spatial imaging device may be any suitable spatial imaging device having a magnetic field. Preferably, the spatial imaging device is an MRI device. Other spatial imaging devices such as PET or CT

devices are suitable for practising the invention. An ultrasound member 4 is engaged with a band 5 which, in turn, is engaged with the head 5 of the subject 1. Only one ultrasound member is shown in Figure 1 but it is possible that more than one member may be used in practising the invention. In electrical communication with the ultrasound member 4 is a conducting lead 6
5 which communicates signals to a pre-amplifier 7 that is located on the side of a magnetic field barrier or shield 8 opposite to the magnetic field 3. The magnetic field barrier 8 operates to shield the pre-amplifier 7 from electrical interference caused by induction of current in the pre-amplifier and conducting lead 6. The conducting lead 6 transverses a second magnetic field barrier 9, which shields the ultrasound-signal analysis device from interference caused by the
10 strong magnetic field 3. It is possible to practise the invention without a second magnetic field barrier. Preferably there are two magnetic field barriers as shown in Figure 1. Preferably, the ultrasound-signal analysis device is a Doppler-Box. The arrangement of the elements herein described allows an ultrasound measurement to be made with the co-operation of the ultrasound elements within and without the magnetic field 3 at a point in time. At alternate
15 points in time, the operation of the ultrasound equipment is paused and spatial images of the subject may be made with the spatial imaging device.

The invention is best performed when the distance between the transducer crystal of the ultrasound member 4 and the pre-amplifier is as short as possible to ensure that adequately
20 measurable ultrasound signals can be acquired. This is achieved by placing the pre-amplifier 7 at the shielded area on the shielded side of the magnetic field shield 7 close to the tissue of interest with a connector for the member. This is best achieved with ultrasound members 4 having long conducting leads 6.

25 The apparatus of the invention includes ultrasound members that may be spatially separate from the ultrasound signal processing and analysing apparatus, preferably including being located in separate rooms to minimise interference from the magnetic field of the magnetic imaging system, wherein the magnetic field shield is a wall of an enclosure such as a room. This is shown in Figure 1 with the magnetic shield 9. In one embodiment of the invention, using
30 an ultrasound Doppler-Box, it is also possible to locate the ultrasound Doppler-Box close to the spatial imaging device.

Any suitable ultrasound member may be used. Preferably the ultrasound members are probes which produce ultrasound waves within the frequency range of 1 MHz to 3 MHz. More

preferably the ultrasound members are 2 MHz to 2.5 MHz ultrasound probes. Figure 2 shows an embodiment of a suitable ultrasound member 4. Preferably, the member 4 contains no electronic elements within.

- 5 Figure 3 shows a side view of the head of a subject 1 with a headband 5 for ultrasound sonication engaged with an ultrasound member 4 in fixed in position for sonication. Preferably, all parts of the headband 5 are constructed of non-magnetic materials.

- 10 Figure 4 shows a front view of the head of a subject 1 with an alternative embodiment of the invention with an ultrasound member 4 on each side of the head of the subject. A conducting lead 6 in conducting communication with the ultrasound member carries signals from each of the ultrasound members.

- 15 It will be understood that the invention is not limited to combining ultrasound apparatus with MRI apparatus but also includes apparatus for other spatial imaging devices including strong magnetic fields such as those implementing CT and PET.

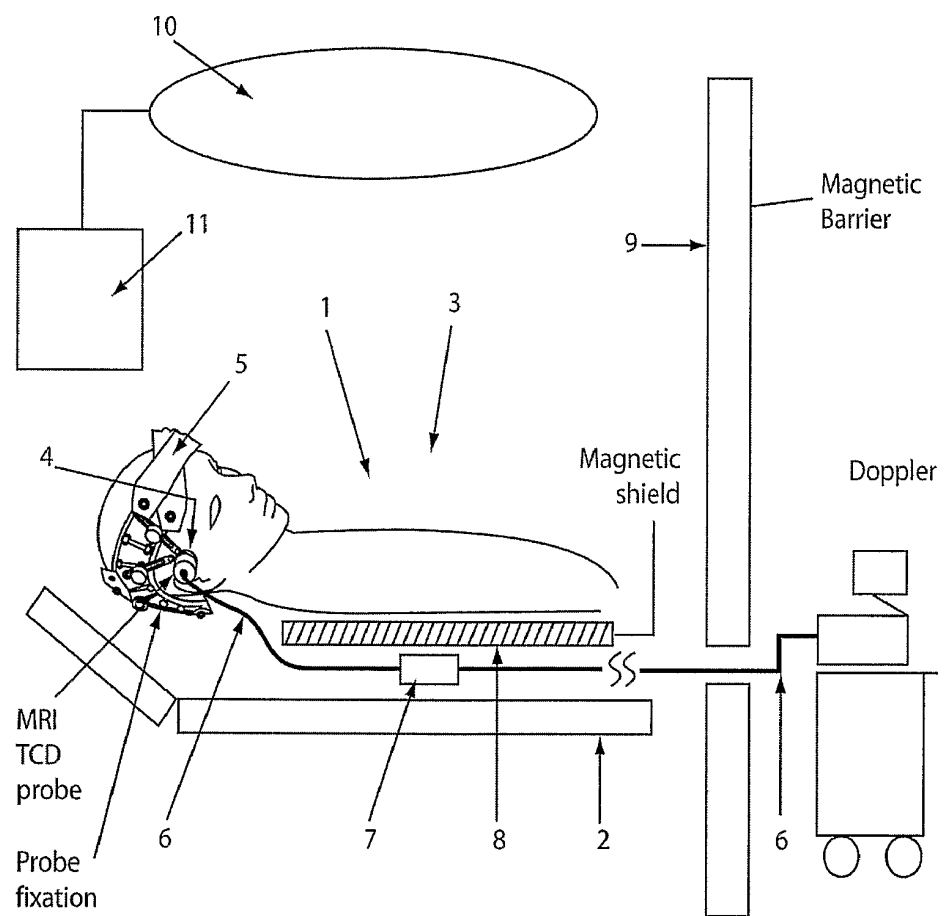
Claims

1. A method of making ultrasound imaging measurement using ultrasound apparatus within the magnetic field of a spatial imaging device having a magnetic field successively with making magnetic spatial images with the spatial imaging device, the method including the steps of:
- 5
- h. positioning at least one non-magnetic ultrasound member adjacent a subject for making an ultrasound measurement;
 - i. establishing electrical communication with the at least one non-magnetic ultrasound member with an ultrasound signal pre-amplifier;
 - 10 j. magnetically isolating the magnetic field of the spatial-image device from said signal pre-amplifying means;
 - k. operating the at least one ultrasound member and an ultrasound imaging means to create a physiological signal of fluid flow in the subject;
 - l. interrupting the operation of the ultrasound member and ultrasound imaging means; and
 - 15 m. operating the spatial imaging device to record an image during said interruption.
2. Apparatus for making ultrasound measurements of fluid flow in a subject located in an imaging device having a strong magnetic field, including:
- 20 a. a least one ultrasound member for generating ultrasound waves, said member having minimal magnetic parts;
 - b. electrical signal communication means in communication with the at least one ultrasound member;
 - c. electrical signal amplifying means;
 - d. magnetic field barrier for magnetically shielding the signal amplifying means; and
 - 25 e. an imaging device having a strong magnetic field wherein said magnetic field barrier is disposed to shield said signal amplifying means from said magnetic field of said imaging device.
3. The apparatus of claim 2 wherein said ultrasound member is an ultrasound probe for
- 30 producing ultrasound waves in the frequency range of approximately 1 MHz to 4 MHz.
4. The apparatus of claim 2 wherein said ultrasound member is an ultrasound probe for producing ultrasound waves in the frequency range of approximately 2.0 MHz to 2.5 MHz.

5. The apparatus of any one of claims 2 to 4 wherein the ultrasound member includes no electronic components.
6. The apparatus of any one of claims 2 to 5 wherein the magnetic field barrier is a wall of an enclosure.
7. The apparatus of any one of claims 2 to 6 further comprising a Doppler box.
8. The apparatus of any one of claims 2 to 7 further comprising a headband for positioning at least one ultrasound member for taking ultrasound measurements.
9. The apparatus of claim 8 wherein said headband is comprised of a non-magnetic material or materials.
10. The apparatus of any one of claims 2 to 9 wherein the conducting parts of the ultrasound member are comprised of carbon materials.
11. The apparatus of any one of claims 2 to 7 wherein said imaging devices is any one of an MRI scanner, PET scanner, or CT scanner.

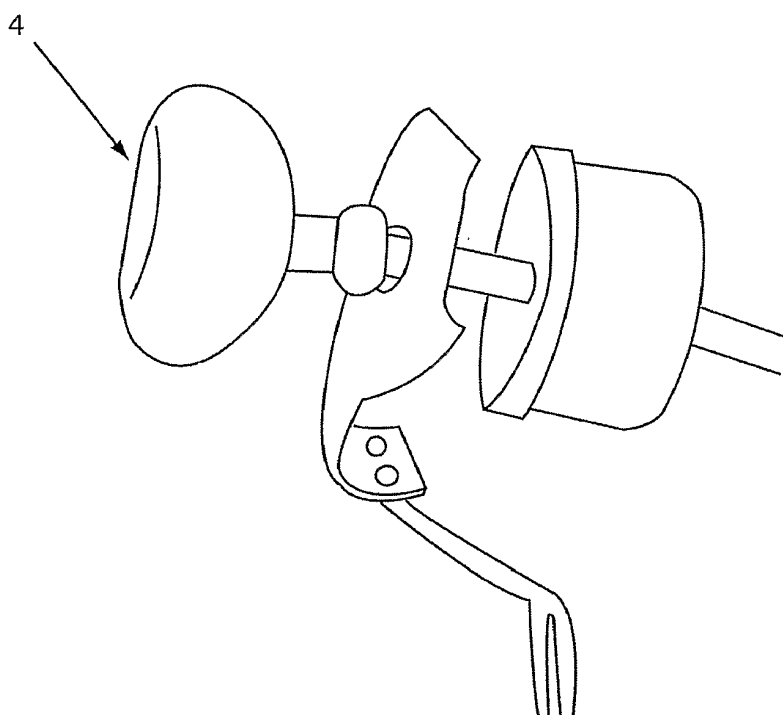
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Figure 1



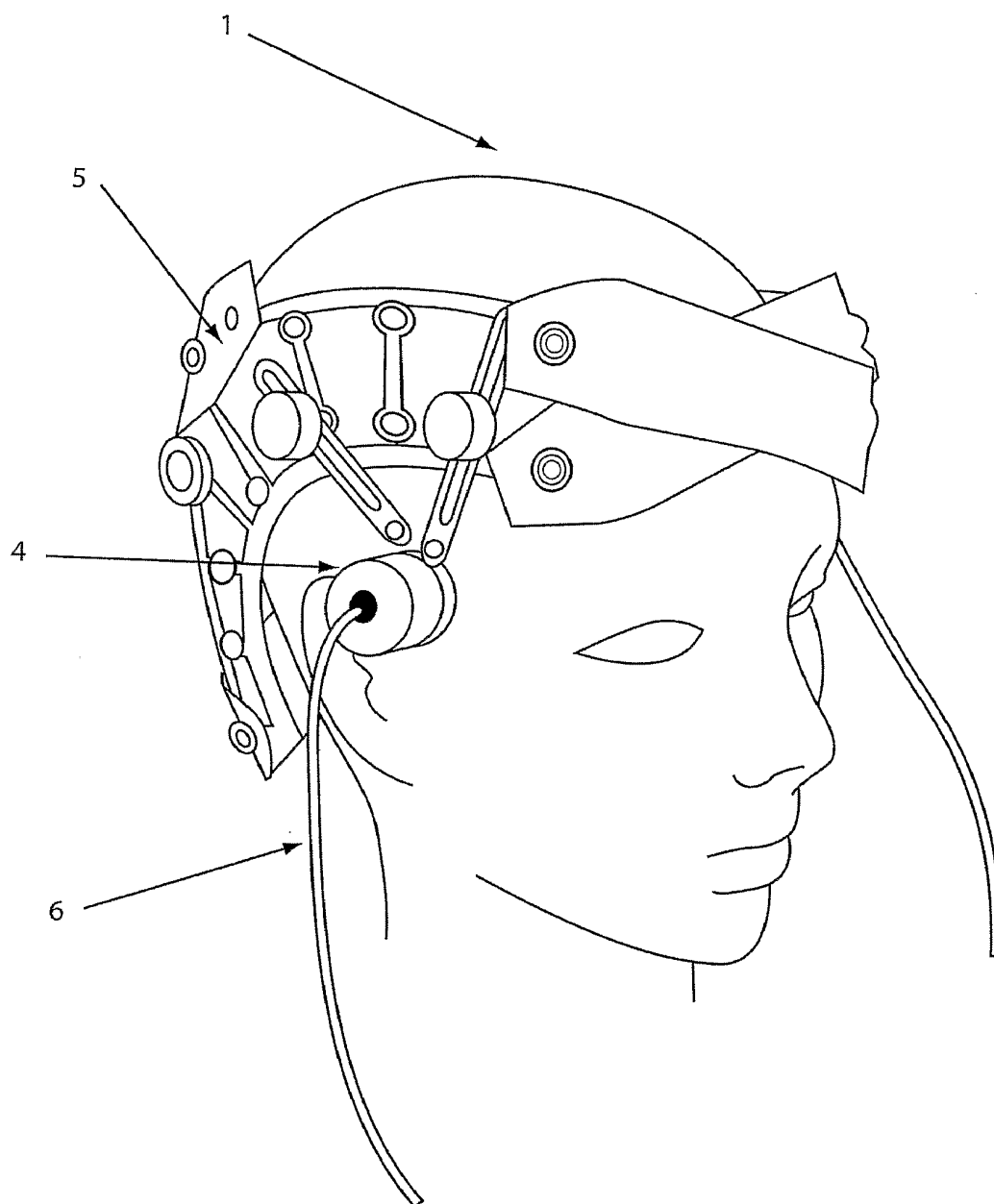
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Figure 2



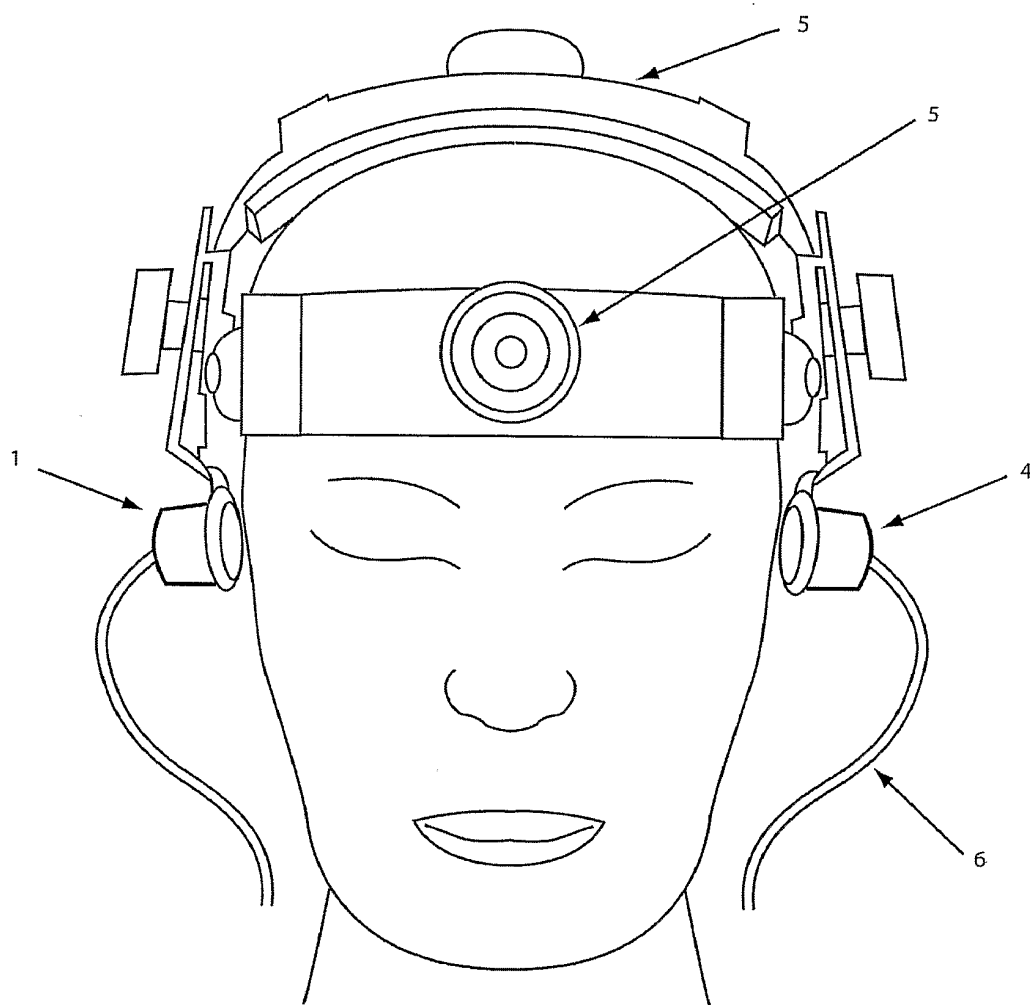
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Figure 3



4/4

Figure 4



INTERNATIONAL SEARCH REPORT

International application No.
PCT/AU2007/000233

A. CLASSIFICATION OF SUBJECT MATTER

Int. Cl.

A61B 5/026 (2006.01)

A61B 8/06 (2006.01)

According to International Patent Classification (IPC) or to both national classification and IPC

B. FIELDS SEARCHED

Minimum documentation searched (classification system followed by classification symbols)

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

Electronic data base consulted during the international search (name of data base and, where practicable, search terms used)

DWPI: IPC A61B and keywords: ultrasound, MRI, imaging, flow, blood, velocity, barrier, shield; and similar terms

C. DOCUMENTS CONSIDERED TO BE RELEVANT

Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X Y	WO 1995/002361 A1 (ZIMMER et al.) 26 January 1995 See entire document	1, 2, 5-11 3, 4
Y	US 5752515 A (JOLESZ et al.) 19 May 1998 See column 3, lines 10-37	3, 4
A	US 5433206 A (SABBAH et al.) 18 July 1995 See abstract and figure 2	



Further documents are listed in the continuation of Box C



See patent family annex

* Special categories of cited documents:

"A" document defining the general state of the art which is not considered to be of particular relevance

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later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention

"E" earlier application or patent but published on or after the international filing date

"X"

document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone

"L" document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified)

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document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art

"O" document referring to an oral disclosure, use, exhibition or other means

"&"

document member of the same patent family

"P" document published prior to the international filing date but later than the priority date claimed

Date of the actual completion of the international search

11 May 2007

Date of mailing of the international search report

17 MAY 2007

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INTERNATIONAL SEARCH REPORT

International application No.

PCT/AU2007/000233

C (Continuation). DOCUMENTS CONSIDERED TO BE RELEVANT		
Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
A	WO 2000/071207 A1 (EXOGEN, INC.) 30 November 2000 See abstract	
A	US 5402789 A (DOW et al.) 4 April 1995 See abstract	
A	US 6280387 B1 (DEFORGE et al.) 28 August 2001 See abstract	
A	Patent Abstracts of Japan, JP 2005-073764 A (HITACHI MEDICAL CORP) 24 March 2005 See abstract	
A	Patent Abstracts of Japan, JP 2003-180696 (OLYMPUS OPTICAL CO LTD) 7 July 2003 See abstract	

INTERNATIONAL SEARCH REPORT

Information on patent family members

International application No.

PCT/AU2007/000233

This Annex lists the known "A" publication level patent family members relating to the patent documents cited in the above-mentioned international search report. The Australian Patent Office is in no way liable for these particulars which are merely given for the purpose of information.

Patent Document Cited in Search Report				Patent Family Member			
WO	1995/002361						
US	5752515	AU	41557/97	AU	42333/97	WO	9807367
		WO	9807373				
US	5433206	DE	19521197	JP	8047496		
WO	2000/071207	AU	50270/00	BR	0010787	CA	2374568
		CN	1361706	EP	1180057	MX	PA01011974
		ZA	200109596				
US	5402789	US	5329194				
US	6280387						
JP	2005073764						
JP	2003180696						
Due to data integration issues this family listing may not include 10 digit Australian applications filed since May 2001.							
END OF ANNEX							

专利名称(译)	磁空间成像装置中的超声波		
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当前申请(专利权)人(译)	COMPUMEDICS有限公司		
[标]发明人	WIDENHORN GEROLD		
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CPC分类号	A61B8/06 A61B5/0035 A61B5/6814 A61B6/03 A61B6/4417 A61B8/0808 A61B8/4227 A61B8/4416 A61B2090/374 G01R33/4814		
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其他公开文献	EP2010049B1 EP2010049A1		
外部链接	Espacenet		

摘要(译)

本发明提供了用于获取超声测量值的装置和方法，所述超声测量值表示来自位于空间成像装置的强磁场中的对象的生物信号。本发明包括具有最小磁性部分的超声探头和超声信号前置放大器，所述超声信号前置放大器被来自空间成像装置（例如MRI，PET或CT扫描仪）的强磁场的屏障屏障屏蔽。最优选地，超声探头产生频率范围约为2.0MHz至2.5MHz的超声波。超声探头可以不包括电子部件并且包含最小的磁性或铁磁部件。用于获取和分析超声波的元件可以位于与成像装置分开的房间中。本发明提供了一种快速连续地进行超声测量的方法，其具有空间成像装置的测量结果，以提供对受试者生理学的更多信息性理解。

