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(54) WIRELESS INTRA-ORAL X-RAY IMAGING

DRAHTLOSE INTRAORALE RÖNTGENBILDGEBUNG

IMAGERIE PAR RAYONS X INTRA-ORALE SANS FIL

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Description

FIELD OF THE INVENTION

[0001] The present invention relates to X-ray imaging, especially to an imaging arrangement used in intra-oral X-ray imaging, to a wireless image sensor and a sensor base station pertaining to it, and to methods for supplying operating power to a sensor and for transmitting data to and from a sensor wirelessly.

BACKGROUND OF THE INVENTION

[0002] Intra-oral X-ray images are taken by using an X-ray examination apparatus which typically includes, on the one hand, a multi-jointed arm construction and a radiation source arranged in connection with it and, on the other hand, an image-data receiving means to be positioned within the patient's mouth in a desired orientation. Generally, electric imaging sensors, which are based on e.g. charge coupled device (CCD) or complementary metal oxide semiconductor (CMOS) technologies, have increasingly emerged along with the use of traditional film.

[0003] In order to enable electric intra-oral imaging, one should be able to, for the first, supply the operating power required by the sensor to be positioned within the mouth and, for the second, transfer the image data detected by the sensor to storage or e.g. onto a display. Furthermore, one must be able to identify in some way the moment of beginning of the imaging at least, i.e., the beginning of irradiation. In the earliest electric intra-oral X-ray arrangements cords were used not only for supplying electric energy but also, *inter alia*, for transmitting signals for synchronising operations of the radiation source and the sensor. Since, solutions have been developed in which e.g. the beginning of irradiation may be identified based on a signal received directly from the sensor, whereby the synchronisation of the operations of the sensor and the radiation source via a cable has not been necessary any more. However, the sensor cable was still required for, on the first hand, supplying electric power and, on the other hand, e.g. transmitting image data and sensor control information.

[0004] In intra-oral X-ray imaging, the sensor has to be repeatedly positioned into different positions within the patient's mouth. In this context the sensor cord bends, whereby the cord itself and its connection to the sensor are repeatedly subject to such forces, which will readily wear out the cord and especially its connection to the sensor. It is quite typical that the lifetime of the cord will be shorter than the one of the sensor itself. Although in intra-oral imaging arrangements the cord as such may, when arranged to be of suitable length, provide a safety means for lessening the possibility of the relatively expensive sensor dropping onto the floor and thus getting broken, one has begun in the field of intra-oral X-ray imaging, as there has been done in many other fields as

well, developing solutions based on wireless technology.

[0005] From the viewpoint of the practical realisation of a wireless intra-oral sensor, an essential characteristic of the sensor is its low power consumption. As it earlier has been possible to achieve diagnostically adequate image quality only with CCD sensor technology, characteristic features of which being fairly high power consumption and complex electronics - not the least because of the several different voltage levels required, a wireless intra-oral X-ray arrangement was not possible to be realised in practice until development of other technologies, such as CMOS sensors, had reached a sufficiently high level.

[0006] A limiting condition of intra-oral X-ray imaging is also the sensor size which cannot, for understandable reasons, be very large both for its surface area and its thickness. On the first hand, one must be able to supply in any case the operating power required by the sensor positioned within the patient's mouth and, on the other hand, transfer the image information detected by the sensor to a display or for storage. In addition, it would be preferable if one would be able to transmit e.g. control signals in the direction of the sensor.

[0007] Thus, in the electric intra-oral sensors of the first-generation the transfer of data and power was realised via cables, as the technology was not advanced enough for wireless data transmission or, overall, for using wireless technology. Wireless arrangements developed since are typically based on using such a base station in which a battery or a capacitor arranged to the sensor is charged either via a physical electric connection to be arranged between the base station and the sensor or by means of induction current. Also replaceable batteries may be used in the sensors. At least a radio frequency (RF) link has been used for transmitting data from the sensor. As far as these prior art solutions are concerned, a reference may be made to e.g. US patent specification 6,527,442 and Japanese published application 2003-79617. The latter of these, for example, describes an imaging arrangement intended to be used in intra-oral X-ray imaging in which a battery or a rechargeable battery, used as the power source of the sensor, is placed in a holder unit outside the sensor, which holder unit is connected to the sensor via a cord. The rechargeable battery may be charged in the base station of the holder unit. Image data may be transmitted from the sensor via the holder unit either when it is connected to its base station or wirelessly by radio technology. The wireless data transmission may be arranged either between the sensor and the base station, or to occur directly together with a personal computer e.g. by Bluetooth technology. If the battery can be realised small enough, it may be placed within the sensor, too.

[0008] Wireless digital intra-oral sensors on the market today have certain characteristics which would be nice to get rid of or be able to be improved. For the first, using batteries as power source of the sensor causes, besides the bother and cost of changing the battery from time to

time, also the fact that it is almost impossible, in practice, to arrange the sensor hermetically sealable in order to enable its cold-sterilisation (immersing it into a liquid). Lifetime of re-chargeable batteries is limited, too, and when using either of them, the sensor inevitably becomes substantially large. For the second, a rechargeable battery or a capacitor must be repeatedly re-charged, whereby one may find oneself in situations in which one has to wait for the sensor to get charged to be ready for imaging - especially when the imaging arrangement should, for reasons of radiation hygiene to begin with, be realised such that the imaging cannot be initiated even, if it is possible that the energy stored in the sensor is not enough for being certain that the picture can be taken and either saved in the sensor itself or sent forward.

[0009] The small sensor size required in intra-oral imaging is problematic also from the viewpoint of wireless data transmission, because RF links realisable with current technology that would enable quick enough transmission of image information and especially bidirectional data transmission are relatively large and require reasonably much power. Using bidirectional RF links also requisites reasonably complicated electronics. On the other hand, if data transmission from the sensor is arranged only unidirectional, e.g. by sending image information from the sensor to the receiver in real time, re-transmitting the image is not possible in case needed but one has to simply trust that there are no disturbances in the data transmission. In data transmission realised by radio frequencies, disturbances may be caused by e.g. the lengthy data transmission distance from the sensor in the patient's mouth (through soft tissue) to the receiver and both GSM phones and other radio transmitters operating at high frequencies (>10 MHz) (Bluetooth, WLAN) or other radio-frequency devices of high-power. In case the power of the power source is not, for some reason, sufficient for performing the imaging event as a whole and transmission of image data is only possible in real time, one may have to repeat the whole imaging.

[0010] The US-A-5 514 873 discloses an x-ray apparatus which has a portable radiation detector having a housing containing a radiation transducer formed of individual detector cells that convert incident radiation, particularly x-radiation, into electrical signals. The radiation detector is implemented cable-free. A wireless transceiver for the infeed of operating energy and for the outfeed of the signals is provided. An energy supply may be arranged in the housing. The energy supply can be implemented as a conventional battery, however, it is also possible to provide a re-chargeable battery that is connected to an electro-mechanical coupling element.

[0011] There may be a need to use a plurality of sensors in the same premises. When using radio frequencies, one might have to use e.g. different frequencies or one has to arrange selectable transmission channels to the sensors for realising undisturbed data transmission. Even then one must in any case be able to manage in some manner which frequency or channel can be used

at a given time.

[0012] An object of the present invention, with its preferable embodiments, is thus to offer possibilities for decreasing or avoiding many of the above-described problems and limitations. Especially, an object of the invention is to decrease the problems related to wireless intra-oral imaging based on batteries, on one hand, and on rechargeable batteries or other components to be charged beforehand for imaging, on the other.

BRIEF DESCRIPTION OF THE INVENTION

[0013] The essential characteristics of the invention are presented in the accompanying patent claims. In the different embodiments of the invention there is no need to charge the image sensor to be ready for imaging beforehand, but the energy required for its use is supplied to the sensor in connection with the actual imaging event. The sensor is arranged to be used without a physical contact to any electric power or data transmission bus and to be activated when it is brought to the operating range of a wireless power transmitter. Preferably, the transmitter sending energy wirelessly to the sensor is integrated with e.g. the source of radiation, whereby when the corresponding receiver is located in the sensor, the arrangement may be realised e.g. in such a way that irradiation is possible only when the sensor is located in the range of the power transmission link in question, which range is arranged short.

[0014] The invention with its preferable embodiments will facilitate the work stages of the dental care personnel external to the actual imaging, as one does not have to take care of changing batteries nor charging the sensor beforehand prior to the imaging event.

[0015] An intra-oral sensor according to the invention may be realised without any lids or slots as hermetically sealed, which enables its sterilisation by immersing in the sterilising liquid, too.

[0016] The imaging arrangement may preferably be realised so that an inductive transmitter is used in power transmission, which transmitter may also be used for supplying data to the sensor. It is also possible to utilise the magnetic field produced by the inductive transmitter in positioning the sensor to a desired position with respect to the X-ray beam produced by the radiation source.

[0017] When arranging the sensor to be operable only in the essential proximity of the power transmitter one may use such an RF link for transmission of image data from the sensor in which the power of the transmitter is considerably low. Further one may accomplish a good immunity against disturbances caused by other devices, such as GSM phones, by using directional antennas and by arranging the receiver of the RF link quite insensitive and/or by placing it inside a beam limiter (of metal) of the X-ray source. Thus, an embodiment of the invention enables a solution in which the data transmission may operate reliably in different operating conditions and more than one sensor may be used within the same space

without them necessarily disturbing each other's operation.

[0018] Especially, the invention enables implementation of the sensor in a relatively small size but, despite of that, as capable of receiving and sending information wirelessly in its imaging position, i.e., to communicate bidirectionally.

[0019] Other objects and some preferable embodiments of the invention will be described in the following in more detail with the aid of the accompanying figures as well. In the following and in the above, when using terms "energy" and "power" in the context of this application is meant, in practice, the same thing, i.e., the "energy" or the "operating power" which must be available for the sensor in connection with the imaging event for enabling imaging.

BRIEF DESCRIPTION OF THE DRAWINGS

[0020]

Figures 1, 2a and 2b show a typical intra-oral X-ray device.

Figure 3 shows components of a sensor and its base station suitable to be used in the imaging arrangement according to the invention.

Figures 4a and 4b show an arrangement according to the invention for realising transmission links.

Figures 5 and 6 show embodiments according to the invention of methods for supplying operating power to the intra-oral sensor in connection with an imaging event.

DETAILED DESCRIPTION OF THE INVENTION

[0021] Figures 1, 2a and 2b show a typical intra-oral X-ray device (1) which includes a control panel (2), a jointed arm construction (3) and an X-ray source (4). Figure 2b shows additionally an elongated collimator (4') which may be attached to a housing of the X-ray source (4) for limiting the X-ray beam more precisely and thus minimising the radiation dose received by the patient. The multi-element arm-joint constructions (3) of intra-oral X-ray devices create a lot of degrees of freedom for positioning the X-ray source (4) in a desired manner.

[0022] Figure 3 shows components of a sensor (30) and a base station (40) suitable to be used in the imaging arrangement according to the invention. Figures 4a and 4b illustrate, for their part, by means of examples how transmission links (33, 43; 36, 46) used in the invention and shown in Figure 3 may be arranged to an intra-oral X-ray device (1) according to Figures 1, 2a and 2b.

[0023] The sensor (30) according to Figure 3 includes an FPGA (field programmable gate array) or an ASIC (application specific integrated circuit) circuit (31) con-

trolling its different functions and a CMOS detector (32). The energy required by the sensor (30) is supplied via a wireless transmission link (33, 43), which in the embodiment according to Figure 3 comprises, on the side of the sensor (30), a receiver (33) of an inductive-link including a coil (34). The coil (34) of the inductive receiver (33) may be arranged e.g. as in the shape of a rectangle so that it essentially imitates the shape of the sensor (30) perimeter and is located in the essential proximity of at least part of the sensor (30) edges. The coil (34) is preferably arranged in connection with the sensor housing so that the winding will not limit the active detector surface available in the sensor. The receiver (33) to be arranged to the sensor may also be e.g. an RF receiver or other corresponding component receiving energy wirelessly and not being electrically chargeable.

[0024] The power supply circuit (35) as such belonging to the sensor (30) may include e.g. small capacitors used in transmitting electric power received from the induction receiver (33) but, according to the invention, the sensor electronics does not include any such component which could be used for storing energy supplied to the sensor (30) beforehand and thus enabling its use without the "on-line power supply" performed in connection with the imaging event via the wireless transmission link (33, 43). The receiver of the transmission-link (33) arranged to the sensor (30) is therefore the primary power source supplying current to the sensor electronics, and the energy storing capacity of the components possibly belonging to the power supply circuit (35) being capable of storing energy is in any case lower than the electric power required by the sensor electronics in connection with an individual imaging event. For example, when considering intra-oral sensors of today, i.e., taking into account, *inter alia*, the detector sizes typically used, e.g. the RF technology used for transmitting image data and the capacitor technologies available, this would mean total energy storing capacity of a capacitor or capacitors possibly belonging to the sensor electronics of below 20 Ws, e.g. below 5 Ws, in practice, easily even an energy storing capacity of less than 1-2 Ws.

[0025] The detector (32) used in the sensor (30) may be monolithic and at least part of the actual sensor electronics may be integrated with it so that already the output from the detector is e.g. in 12-bit digital form. Even though part of the active detector area will be lost as a consequence of such increase of electronics, the loss may be minimised by arranging the main portion of the components to one end of the detector (32) and to the other three sides only that portion of the electronics which is necessary. In case CMOS technology is used, the power requirement of the sensor (30) is relatively low. With advancing technology, it is presumable that one will be able to integrate the whole FPGA or ASIC circuit (31) with the detector (32). On the other hand, with advancing detector technology it is presumable that a sensor with such preferable characteristics which are presented as advantages of the CMOS technology here when using it in an

application according to this invention will be realisable also with other solutions than the ones based on CMOS technology.

[0026] Image information is transmitted from the sensor according to Figure 3 by an RF transmitter (36) of 2.4 GHz, either essentially in real time as image data is detected on the detector (32) (so-called streaming mode) or essentially immediately after the image has been taken. It is possible to arrange e.g. a RAM (random access memory) or a FLASH memory (38) to the sensor (30) for temporarily storing the detected image, whereby it can also be re-sent in case so required. The size of the memory may be arranged to enable storing of either the image data as a whole or only part of it. In the latter case, the imaging arrangement is preferably implemented so that there has been arranged a means to the base station (40) for identifying the data packets possibly damaged in transmission and a means for transmitting information of this quickly to the sensor (30). This is possible e.g. by using the energy transmission link (33, 43) for this data transmission and by arranging the speed of it to be sufficient. In even more general terms, thus, the energy transmission link (33, 43) may be used for transmitting to the sensor (30) both energy and information.

[0027] Figure 3 shows also a preferable solution for a base station (40) according to the invention. In the context of this invention, a base station means primarily a functional entity which may be arranged not only as a single physical unit, but its components or part thereof may also be integrated partly or completely with other construction(s) or device(s), such as a radiation source or an image processing device. The energy needed for operating a sensor (30) in connection with an imaging event is transmitted to it via the inductive transmitter (43) of the base station (40) shown in Figure 3. As already referred to above, the inductive link (33, 43) may also be used for data transmission in the direction of the sensor (30). Then again data, such as image and status information that has been transmitted by the sensor (30) will be received at the RF receiver (46) arranged to the base station (40). By arranging to the imaging arrangement bidirectional data transmission according to Figure 3 by means of, first, an unidirectional RF link (36, 46), and second, an inductive link (33, 43) one will be able to use unidirectional RF links which are considerably smaller and simpler than bidirectional RF links that, for its part, enhances possibilities for realising the sensor (30) as small in size.

[0028] It is possible to implement the invention so that significantly lower data transmission speed is used for sending control data to the sensor (30) than what is required in practice for transmitting image data from the sensor (30), but also e.g. an inductive link (33, 43) may be realised such that also a high-speed data transmission is enabled. Then, it can be utilised e.g. in the above-described manner for transmitting error messages to the sensor (30) while image data is being transmitted in a situation in which one of the transmitted data packets has been damaged. Data transmission errors are actually

not a real problem when such a large memory (37) is arranged to the sensor (30) that the whole image data may be re-transmitted in case needed, but by arranging the data transmission connections such that information of the damaged data packet will be transmitted to the sensor (30) in time, in view of enabling re-transmission of the data packet still in the memory (38), it is sufficient to use also a smaller memory.

[0029] The base station (40) according to Figure 3 also includes a base-station power supply circuit (45), an FPGA circuit (41) transmitting image data to the processor (49) of the base-station and a memory (48) functioning in connection with the processor, which memory enables temporary storing of image-data received from the sensor (30). In addition, there has been arranged Ethernet and/or USB (Universal Serial Bus) user interfaces (61, 62) to the base station (40) via which one is able to connect e.g. to an image processing device, a patient management system of a dental clinic etc. connected to a local area network. Furthermore, the base station may be arranged with a data transmission connection, not shown in Figure 3, via which the operation of the radiation source (4) and the sensor (30) may be synchronised, if so desired, such that the control system of the imaging arrangement is arranged to prevent use of the radiation source (4) unless the sensor (30) used in imaging is located within the operating range of the power transmission link (33, 43), i.e., unless the sensor (30) is ready to receive radiation including image information. Naturally, the components of a base station (40) according to or corresponding to that of Figure 3, or part thereof may also be e.g. an integrated part of electronics of a radiation source (4) or be divided physically to even more than one unit.

[0030] In the arrangement according to the invention, the base station (40) may take the power it requires from the bus (Power-LAN, USB) via which image data is transmitted forward to a personal computer (PC) or a data network, whereby one avoids using an external power source needed for this purpose only. There may be circumstances, though, in which such a preferable and simple solution is not adequate, in light of which the base station (40) may be provided with a connection of its own for an external power source.

[0031] Figures 4a and 4b, especially Figure 4a, illustrate one preferable embodiment of the invention in which the coil (44) of the inductive transmitter (43) and the RF receiver (46) together with its antenna (47) have been physically separated from the actual base station (40) to form an adapter or a transponder (70) of e.g. circular or rectangular form and being connectable to the X-ray source (4), e.g. to a collimator (4') attached thereto, and being connected to the electronics of the actual base station (40) via a cord (71). The RF receiver (46) with its antenna (47) shown in Figure 4a has been left out of Figure 4b for simplicity's sake, and Figure 4b has been correspondingly complemented compared to Figure 4a to show also how the sensor (30) would be typically po-

sitioned in connection with an imaging event with respect to the transponder (70) according to Figure 4a. So, if also the sensor (30) and e.g. the collimator (4') of the radiation source (4) were drawn in figure 4a, the sensor (30) would be located to the left of the transponder (70) and the collimator (4') would converge to the transponder (70) from the right.

[0032] In the embodiment according to Figures 4a and 4b the coil (44) of the inductive transmitter (43) is thus arranged within a ring-shaped adapter or transponder (70), and also the antenna (47) of the RF receiver (46) and its preamplifier (not shown in the figures) are integrated with the adapter (70). The adapter (70) may be attached to the end of e.g. an X-ray tube head (4) or a collimator tube (4') used in it. In such an arrangement, the transmission links (33, 43; 36, 46) will always become positioned to roughly the same distance, such as around 2-8 cm, and in the same direction with respect to each other in connection with imaging when the imaging arrangement (50) is ready for imaging, i.e., when the intra-oral sensor (30) is positioned in the patient's mouth and the X-ray source (4) is located in its corresponding imaging position. *Inter alia*, in such embodiment of the invention, one is able to use directional antennas (37, 47) for transmitting image data which, for its part, improves noise immunity of the data transmission system. It is also possible to place the antenna (47) of the RF receiver inside the collimator tube (4') in order to protect it from external sources of disturbances. When, in addition, the distance of data transmission between the RF link (36, 46) antennas (37, 47) will therefore be short, the transmission power it requires will also be low. The data transmission distance is thus in practise e.g. less than 15 cm, such as in the order of 2-8 cm. It is possible to arrange the RF receiver (46) receiving image information less sensitive and thus make the data transmission relatively immune to the effects of possible sources of disturbances. The short transmission distance also enables that interference will not be created from the other sensors possibly being in use and thus there is no need to code the sensors to different channels.

[0033] Concerning the energy transmission, the intra-oral X-ray imaging arrangement according to the invention is preferably realised such that in connection with the imaging situation the transmitter (43) supplying energy to the sensor (30) is arranged to always become positioned in the essential vicinity of the sensor (30) positioned in the patient's mouth. Such positioning objects are e.g. a holder arranged on the patient's neck, ear or a band on his/her forehead or a corresponding item, or e.g. on the headrest of the dental chair or, as said, the X-ray source (4) itself.

[0034] In connection with intra-oral X-ray imaging one typically aims to collimate (limit) the X-ray beam to correspond the shape and size of the image-data receiver used and to position the image-data receiver at the centre of the beam; this situation being illustrated also in Figure 4b. One preferable embodiment of the invention thus

comprises an arrangement in which the inductive transmitter is placed within the X-ray source and in which small receiver coils are arranged e.g. essentially to the corners of a sensor (30) of essentially of rectangular shape, or to at least one of them. When the sensor (30) is being positioned with respect to the radiation source (4) - or in connection with intra-oral imaging, more frequently perhaps *vice versa*, when the X-ray source is being positioned with respect to the sensor - the signals received from the coils change according to how their position changes in the magnetic field produced by the inductive transmitter (43) attached to the X-ray source (4). These signals may be arranged to be sent e.g. via the RF link (36, 46) as signals indicating the relative positions of the sensor (30) and the X-ray source (4), which signals may be utilised in achieving the desired relative position of the sensor (30) and the radiation source (4). Naturally, it is possible to receive more data from several of such coils compared to only one coil. However, it is possible to arrange a corresponding signal from a receiver (33) of the inductive link (33, 43) only, which receiver essentially circles the edges of the sensor (30), whereby even it alone can be used to facilitate in positioning the sensor.

[0035] The wireless data transfer of intra-oral imaging may thus be realised so that e.g. a sensor including a CMOS detector will communicate wirelessly bidirectionally with a base station into which base station, or into functional connection thereof is also arranged a means for wireless energy transmission. In connection with imaging, the energy required for data transmission and for operation of the sensor in general is supplied to the sensor by bringing a transmitter supplying energy and a sensor comprising a corresponding receiver within the operating range of the link formed by them, preferably into the essential vicinity of each other, such as within an operating range arranged to be of less than 50 cm, preferably less than 15 cm, such as 2-8 cm. Then, when the sensor in itself has no such energy-storing components that would enable use of the sensor without energy transmission during the imaging event, it is possible to use the sensor only when it is located substantially close to the transmitter of the energy transmission link. The operating power required by the sensor is preferably transmitted inductively, whereby the inductive transmitter is preferably placed e.g. in connection with the end of the intra-oral X-ray tube head, e.g. to the tube-like part of its housing, or to the adapter to be positioned at the end of the collimator connected to it. The inductive transmitter may also be integrated e.g. as a part of the construction of the X-ray source.

[0036] In connection with the imaging event the operating system of the imaging arrangement identifies that the sensor is brought into the operating range of the power transmission link and the imaging may be started. The field of inductive power transmission may be arranged to be of relatively low frequency for minimising the possible disturbing effects it may have to the operation of the imaging sensor. The frequency used in the transmis-

sion may be e.g. essentially lower than 500 kHz, even totally of a different order of magnitude.

[0037] If the arrangement will be implemented so that the sensor will nevertheless be able to momentarily operate without continuous external energy supply, the energy transmission may be momentarily interrupted or adjusted lower in connection with the imaging event e.g. for the duration of the actual exposure, for the duration of reading image data from the detector to a memory possibly arranged to the sensor, or when sending it from the sensor to the ether. In such an application it may be preferable to implement the arrangement so that the power of the energy transmission link is arranged lower than the power taken by the (RF) transmitter link used in transmitting image data. A momentary interruption of the energy transmission may have an enhancing effect in that the power transmission taking place during an imaging event will not cause disturbances to the operation of the sensor. On the other hand, a means may be arranged to the sensor itself, too, for adjusting its power consumption at different stages of the imaging event.

[0038] Thus, according to one embodiment of the invention, it is possible to store the image data detected by the detector temporarily to a memory arranged to the sensor and to transmit it for storage from the detector after the exposure has finished, preferably as quickly as possible. This may be realised e.g. in such an arrangement in which the time the irradiation ends is known beforehand or it is identified. However, it is possible to read the signal of particularly e.g. a CMOS-type detector continuously also during the exposure. The sensor may then be arranged usable also in the so-called streaming mode, i.e., so that image data is transmitted from the sensor continuously during exposure. It will then be later possible to detect the beginning and the end of the exposure by software e.g. from the signal stored in the PC's memory. When image data is transmitted in real time at the same rate as it is read, e.g. at 300 ms intervals, there is no need to know the maximum exposure time from the viewpoint of image formation, when the data possibly causing overexposure may simply be ignored in image processing.

[0039] All in all, according to the invention, energy is supplied to the sensor essentially only in connection with the imaging event, i.e., starting a little earlier than the actual exposure is initiated, such as when positioning the imaging means for the exposure, for example, and until the image data has been managed to be transmitted from the sensor - or stored to the memory arranged in the sensor.

[0040] If image data is transmitted from the sensor only after exposure and no memory has been arranged in the sensor for storing image data, naturally, the power transmission link may not be brought outside its operating range before image data has been managed to be sent from the sensor. For preventing this, it is possible to arrange an indication light or other signal in connection with e.g. the inductive transmitter, such as to the intra-oral X-

ray source in the embodiment according to Figure 4b, which signal will indicate after the imaging that transmission of image information has been completed. When using a sensor provided with memory, it is naturally also possible to stop the transmission of the data, to do it later after imaging and/or transmit the data more than once in case the data transmission has in some way or another failed. Considering subsequent data transmission, it is possible to arrange a holder e.g. in connection with the X-ray tube, to which the sensor may be placed after imaging to enable communication with the base station arranged to the X-ray tube still after the actual imaging. In transmitting data from the sensor, a high-frequency radio transmitter and e.g. transmit power of the order of less than 1 mW are preferably used for minimising the effect of transmission on the operations of the CMOS detector and the digital electronics of the sensor.

[0041] Figures 5 and 6 show two examples of how the invention may be applied in practise in connection with intra-oral X-ray imaging. Figure 5 shows the use of the invention in a manner in which mutual operation of the radiation source and the energy transmission link have been synchronised. According to this embodiment, in the first stage when power of the X-ray source is turned on, the arrangement enters a STAND BY mode. The preparation stage of the imaging may include, *inter alia*, positioning of the radiation source, the object to be imaged and the sensor, ready for imaging. Then, when upon initiating the actual imaging an irradiation start signal is given from the exposure switch of the radiation source, the system first activates the transmitter of the energy transmission link according to the invention and checks if there is such a sensor unit within the operation range of the link which the system recognises. (As all sensors are individuals and their use requires knowledge of the sensor-specific calibration data, it is possible to use in the imaging only such sensors the repair (calibration) file of which is stored to a database pertaining to the imaging arrangement in order that one will be able to form from the image data detected by particularly that sensor in question a "real" image representing the object. With an individual serial number, it is also possible to prevent an unauthorised use of the sensor and make stealing of it pointless by user-specific opening code.) In practice, the identification of the sensor takes place so that, when being located within the operating range of the energy transmission link, the sensor sends a signal including its individual identifier via a data transmission link pertaining to the arrangement as a response to its activation. If the identifier in question is not stored to the system, i.e., if one tries to use such a sensor the databases used by the imaging arrangement do not identify, or if e.g. the respective distance between transmitter and receiver of the power-transmission-link is greater than the operating range of the link, or if the system detects some other error in the imaging arrangement, irradiation does not start and the system gives an error signal, such as a sound signal, and informs of the cause of the error. A cause of the error

signal may also be e.g. inaccurate positioning of the sensor with respect to the X-ray beam produced by the radiation source.

[0042] When preconditions for a successful imaging exist, that is, *inter alia*, the energy transmission link transmits energy to the sensor it has identified and the sensor electronics has been activated ready for imaging, then e.g. the EXPOSURE light belonging to the arrangement is turned on, and if no exposure automatics for the imaging are included in the arrangement, irradiation of a preset duration starts. After the irradiation, the EXPOSURE light is turned off. After the exposure, the arrangement may still enter a separate BUSY mode the duration of which may depend on, for example, how transfer of the image data detected by the detector element is arranged to occur, *i.e.*, if there is arranged a memory to the sensor via which the transfer may be done partially or as a whole also after the exposure, if there has been arranged, in connection with the transfer, feedback to transmit to the sensor information regarding data packets that may have been damaged etc. The transfer of image data may thus also be realised so that the data detected by the detector is first stored to a memory in the detector, after the imaging the sensor is transferred e.g. to a holder arranged in connection with the base station, *i.e.*, to a position in which it is within the operating range of the power transmission link, and image data is transmitted from the sensor only at this stage. After transfer of the image data, indication lights turn off, the energy transmission link inactivates and the system returns to the STAND BY mode.

[0043] Figure 6 shows an example of an embodiment in which the energy transmission link and the radiation source function independently with respect to each other. In this solution, the base station of the energy transmission link communicates with e.g. a PC, and when being in the STAND BY mode, the transmitter of the energy transmission link periodically sends short pulses to the ether, whereby as a response to the signal of finding a sensor within the operating range of the arrangement, the operation mode of the transmitter changes from said periodical-pulse-sending mode to an actual READY mode and the sensor is activated ready for imaging. For the sake of simplicity, in the diagram according to Figure 6 the alternative that one would try to use some other sensor individual than such known by the system, and also other possible error situations shown in connection with the embodiment according to Figure 5, have been omitted. If no actual exposure is done e.g. within a time preset to the system from the time the system went to the READY mode, that is, *i.e.*, if no signal will be received from the sensor within such time of the start of irradiation, the system returns to the STAND BY mode as described above. Such a situation may occur e.g. when an exceptionally long time elapses for positioning of the sensor and the radiation source for imaging.

[0044] Detecting the start of irradiation causes a change of the status of the system to an EXPOSURE

mode, during which the information detected by the detector will be integrated e.g. for a pre-determined time or until the end of irradiation is detected. If the arrangement is implemented so that the data detected by the detector is read by short intervals continuously from the detector already during the exposure, the detection of the end of irradiation may be based on an observation of a sudden fall of the detected signal level. The transmission of image data from the sensor may also be realised e.g. in some manner presented above in connection with the description of Figure 5, after which the EXPOSURE (or BUSY) indication light is turned off and the arrangement returns to the STAND BY mode.

[0045] The invention is described here particularly in connection with its primarily preferred application, intra-oral X-ray imaging. In principle, it is possible to bring the operating power required by the sensor from outside the sensor with some other wireless technology than inductively as according to the embodiments described above, and in principle, by using only one link for transmitting both energy (and data) to the direction of the sensor and, on the other hand, for transmitting image data from the sensor. However, an arrangement according to the above-described embodiments, in which the energy is supplied to the sensor inductively and image data is transmitted in radio frequencies, respectively, enables an energy transmission/bidirectional data transmission assembly exquisitely applicable for intra-oral imaging. Then, it is also possible to construct the imaging arrangement such that the magnetic field formed by the power transmission link may also be utilised in positioning the sensor with respect to the X-ray source, as described above.

[0046] According to one preferable embodiment of the invention, the sensor data transmission is thus bidirectional and realised e.g. so that image and status data is sent from the sensor with high rate (such as at least 10 Mbit/s) with an essentially high-frequency RF transmission link of e.g. 2.4 GHz, and the sensor receives energy inductively, whereby the inductive link may also be used for slower (such as less than 9,600 kbit/s) communication in the direction of the sensor, such as for sending the sensor control signals.

[0047] The lifetime of a sensor according to the invention is long as there is no need to arrange into it any components which would be large in size, wear out when used or age or be replaceable, such as batteries or rechargeable batteries. Actually, almost the only possibility for the sensor according to the invention getting broken is a mechanical breakage caused by too a high external mechanical strains, such as a physical impact caused by the sensor dropping onto the floor or a physical impact caused by another corresponding accident. The risk of dropping onto the floor may be prevented by e.g. a safety cord and a small lug arranged to the back cover of the sensor or by other corresponding fastener arrangement. If one uses a string manufactured of thin Kevlar fibre or nylon line it can be cold-sterilised together with the sen-

sor, or one may use disposable strings. Then, it is not necessary to use the protective bags typically used for hygienic reasons with a sensor according to the invention.

[0048] Thus, the arrangements according to the invention and its preferable embodiments provide new kinds of possibilities for implementing a wireless intra-oral sensor. For example, the use of a high-frequency and unidirectional RF link for data transmission enables a simpler sensor construction which can be realised smaller in size and the control of which is also notably simple. Because of the short transmission range, also the power consumption of the data transmission link is low, whereby also the amount of energy that has to be transmitted to the sensor is low. The use of short transmission range and a high-frequency data transmission link enable realisation of the invention without sophisticated unique application-specific arrangements, by using prior art solutions which have proven to be functional. It is also possible to arrange the data transmission channel as relatively immune to external disturbances. The components of the RF link may be realised either with discrete parts or as an integrated circuit, the use of neither disturbing the inductive link of the other direction pertaining to the arrangement when the links use essentially different frequency bands. If desired, the image data may be transmitted in real time.

[0049] With a sensor construction according to the invention, which does not include a battery, a rechargeable battery or corresponding pre-chargeable component designed for storing operating energy of the sensor, it is possible to realise the sensor as small in size, when using the sensor there is no need to repeatedly replace the battery, or charge the re-chargeable battery, nor does there exist any problems caused by ageing of the rechargeable battery, taking care of servicing the sensor components, mechanical or other damages or charging the sensor between imagings. The sensor may also be realised hermetically housed and galvanically insulated, which enables its cold-sterilisation between imaging of different patients.

[0050] It is well known for a man skilled in the art that the present invention may be realised within the scope of protection defined by the accompanying patent claims also according to other embodiments than the ones presented above, *inter alia*, along with new possibilities offered by the advancement of detector technology.

Claims

1. An intra-oral X-ray imaging arrangement comprising:
 - a control system;
 - a radiation source (4) which is arranged e.g. in connection with a jointed arm construction (3);
 - an electric image data receiver (30) such as e.g. a sensor based on CMOS technology; and

a wireless transmission link (33, 43; 36, 46) for transmitting at least image data detected by the electric image data receiver (30) to a base station (40) of the electric image data receiver (30), to an image processing device or to a corresponding other device capable of receiving image information, the transmitter and the receiver of which transmission link (33, 43; 36, 46) are arranged, on the one hand, in connection with the electric image data receiver (30), and on the other hand, at least in functional connection with said base station (40),

characterised in that

the arrangement further includes a wireless power transmission link (33, 43), which wireless power transmission link (33, 43) is arranged for the use of supplying the electric image data receiver (30) with energy in connection with an imaging event.

2. An imaging arrangement according to claim 1, **characterised in that** a receiver (33) of said power transmission link (33, 43) is arranged as a part of electronics of the electric image data receiver.
3. An imaging arrangement according to claim 1 or 2, **characterised in that** a receiver (33) of the power transmission link (33, 43) pertaining to electronics of the electric image data receiver is the primary power source of a power supply circuit (35) pertaining to the electronics.
4. An imaging arrangement according to any one of claims 1-3, **characterised in that** the receiver of the power transmission link (33, 43) is an inductive (33) or an RF receiver (46), or such a corresponding component receiving electro-magnetic energy wirelessly which is electrically non-chargeable.
5. An imaging arrangement according to any one of claims 1-4, **characterised in that** it includes a means for transmitting to the electric image data receiver (30) energy it requires in connection with an imaging event wirelessly during the actual imaging event.
6. An imaging arrangement according to any one of claims 1-5, **characterised in that** the total energy storing capacity of component(s) possibly pertaining to electronics of the electric image data receiver that are capable of storing energy is lower than the energy required by the electric image data receiver (30) in connection with an individual imaging event.
7. An imaging arrangement according to claim 6, **characterised in that** the total energy storing capacity of component(s) possibly pertaining to the electronics that are capable of storing energy is lower than

20 Ws, such as lower than 5 Ws.

8. An imaging arrangement according to claim 7, **characterised in that** the total energy storing capacity of component(s) possibly pertaining to the electronics that are capable of storing energy is lower than 1-2 Ws.
9. An imaging arrangement according to any one of claims 1-8, **characterised in that** the operating range of said power transmission link (33, 43) is arranged short, such as less than 50 cm, preferably less than 15 cm, such as 2-8 cm.
10. An imaging arrangement according to claims 1-9, **characterised in that** the transmitter (43) of said power transmission link (33, 43) is placed or arranged to be placed in a location or a position in which, when the object to be imaged and said electric image data receiver (30) are positioned to their imaging positions according to the imaging arrangement (50), the electric image data receiver (30) is positioned within the operating range of the power transmission link (33, 43).
11. An imaging arrangement according to claim 10, **characterised in that** the transmitter (4) of the power transmission link (33, 43) is arranged to be placed to a radiation source (4) or a base station (40) arranged in essential connection with it, or e.g. a base station (40) attachable to the patient or arranged to the headrest of a dental chair.
12. An imaging arrangement according to any one of claims 1- 11, **characterised in that** it includes a means for transmitting a signal from the electric image data receiver (30) as a response to the electric image data receiver (30) and the transmitter (43) of the power transmission link (33, 43) being located within the operating range of the power transmission link (33, 43).
13. An imaging arrangement according to claim 12, **characterised in that** it includes a means for synchronising the operations of said power transmission link (33, 43) and radiation source (4) so that irradiation cannot be started if the control system of the imaging arrangement (50) has no information on the receiver (33) of the power transmission link (33, 43) arranged to the electric image data receiver (30) being located within the operating range of the power transmission link (33, 43).
14. An imaging arrangement according to any one of claims 1-13, **characterised in that** a means has been arranged thereto for controlling the power transmitted to the electric image data receiver (30) during an imaging event and/or used by the electric

image data receiver (30) during an imaging event.

15. An imaging arrangement according to any one of claims 1-14, **characterised in that** it includes a means for bidirectional data transmission between the receiver of image data and the control system of the imaging arrangement (50), which data comprises at least control commands and image data detected by the receiver of image data.
16. An imaging arrangement according to any one of claims 1- 15, **characterised in that** said power transmission link (33, 43) is arranged to transmit during the imaging event both energy required by the electric image data receiver (30) and control signals of the electric image data receiver (30).
17. An imaging arrangement according to claim 16, **characterised in that** said power transmission link is an inductive link (33, 43).
18. An imaging arrangement according to claim 17, **characterised in that** the receiver (33) of said inductive link (33, 43) comprises a coil (34) essentially imitating the shape of the electric image data receiver (30) perimeter and being located at least in part in the essential vicinity of the edges of the electric image data receiver.
19. An imaging arrangement according to claim 17 or 18, **characterised in that** one or more relatively small coils are arranged to said receiver of image data so that they are located, for example, in the essential proximity to at least one of the corners of the receiver of image data of essentially of rectangular shape, which coil or coils are arranged to transmit data on the position of said receiver with respect to the transmitter (43) of said inductive link (33, 43) in the magnetic field produced by it.
20. An imaging arrangement according to any one of claims 1- 19, **characterised in that** said wireless transmission link (36, 46) for transmitting at least the image data detected by the electric image data receiver (30) is an RF link.
21. An imaging arrangement according to claim 20, **characterised in that** said RF link (36, 46) is a unidirectional link and/or a high-frequency link and/or directional antennas are used in it.
22. A wireless electric receiver of image data, such as a sensor, especially for use in connection with intra-oral X-ray imaging, which receiver comprises a housing and electronics arranged therein, which electronics include a detector (32) based on e.g. CMOS technology, a transmitter for transmitting at least the image data detected by said detector (32) to the ether

and a power supply circuit (35),

characterised in that

the power supply circuit further includes a receiver (33) of a wireless power transmission link (33, 43), which receiver (33) includes and/or in a functional connection of which is arranged a means for receiving and transmitting energy in connection with an imaging event.

23. A wireless electric image data receiver according to claim 22, **characterised in that** it includes a means for transmitting a signal from the wireless electric image data receiver (30) as a response to it being brought to the operating range of said power transmission link (33, 43), which signal may also comprise identifying data of the wireless electric image data receiver in question.
24. A wireless electric image data receiver according to claim 22 or 23, **characterised in that** said receiver (33) of the power transmission link (33, 43) is an inductive or an RF receiver, or such a corresponding component receiving electro-magnetic energy wirelessly, which is electrically non-chargeable.
25. A wireless electric image data receiver according to any one of claims 22-24, **characterised in that** the energy storing capacity of the components possibly pertaining to the power supply circuit (35) that are capable of storing energy is lower than the energy required by the wireless electric image data receiver (30) in connection with an individual imaging event.
26. A wireless electric image data receiver according to claim 25, **characterised in that** the total energy storing capacity of the condenser(s) possibly pertaining to the electronics that are capable of storing energy is lower than 20 Ws, such as lower than 5 Ws.
27. A wireless electric image data receiver according to claim 26, **characterised in that** the total energy storing capacity of the condenser(s) possibly pertaining to the electronics is lower than 1-2 Ws.
28. A wireless electric image data receiver according to any one of claims 22-27, **characterised in that** a means has been arranged to the wireless electric image data receiver (30) for controlling the power it receives and/or uses in connection with an imaging event.
29. A wireless electric image data receiver according to any one of claims 22-28, **characterised in that** said receiver (33) of the power transmission link (33, 43) is an inductive receiver (33).
30. A wireless electric image data receiver according to claim 29, **characterised in that** said receiver (33) of the inductive link (33, 43) comprises a coil (34) essentially imitating the shape of the wireless electric image data receiver (30) perimeter and is located at least in part in the essential vicinity to the edges of the wireless electric image data receiver.
31. A wireless electric image data receiver according to claim 30, **characterised in that** a means has been arranged in functional connection with said coil (34) for measuring and transmitting information on the strength of the magnetic field formed by the transmitter (43) of the inductive link (33, 43) which transmits power to the wireless electric image data receiver (30).
32. A wireless electric image data receiver according to any one of claims 22-31, **characterised in that** it is a sensor (30) of essentially rectangular form, into essential proximity to at least one corner of which rectangle is arranged a coil, in functional connection with which is arranged a means for measuring and transmitting information on the strength of the magnetic field formed by the transmitter (43) of the inductive link (33, 43) which transmits power to the sensor (30).
33. A wireless electric image data receiver according to any one of claims 22-32, **characterised in that** the electronics include a means for receiving control data possibly transmitted in connection with said wireless power transmission.
34. A wireless electric image data receiver according to any one of claims 22-33, **characterised in that** the component of it transmitting image data is an RF transmitter (36), especially a high-frequency, such as 2.4 GHz, unidirectional RF transmitter (36) including a directional antenna.
35. A wireless electric image data receiver according to any one of claims 22-34, **characterised in that** the electronics include a means for storing at least part of the image data detected by the detector (32) in a memory (38, 48) pertaining to the electronics, such as a RAM or FLASH memory, simultaneously while image data is still being detected or essentially immediately after ending the reception of image data.
36. A wireless electric image data receiver according to claim 35, **characterised in that** the electronics include a means for re-transmitting the image data, or part of it, stored in said memory (38, 48), as a response to a control signal which is received by the wireless electric image data receiver (30) wirelessly, such as via said receiver (33) of the link (33, 43) used in power transmission.
37. A base station for an intra-oral X-ray sensor, which

comprises components in functional connection with each other forming a base station (40) electronics arrangement, which components include a component wirelessly receiving at least image data from a sensor (30) used in X-ray imaging,

characterised in that

the base station (40) further includes a means to wirelessly transmit to the sensor (3) energy it requires in connection with an imaging event, as a response to a signal received from said sensor (30) in connection with the imaging event, according to which signal the sensor (30) is located within the operating range of said link (33, 43).

38. A base station according to claim 37, **characterised in that** said signal is arranged to be attained from the sensor (30) as a response to a signal received by the sensor (30) being sent from the base station (40).

39. A base station according to claim 38, **characterised in that** a means is arranged to the base station (40) to verify if said signal includes a recognisable identifier, which will identify the sensor (30).

40. A base station according to any one of claims 37-39, **characterised in that** the electronics of the base station (40) are arranged in functional connection with a radiation source (4) used in imaging so that the use of the radiation source (4) will be prevented if the arrangement control system has no data on said sensor (30) used in imaging being located within said operating range of the link (33, 43).

41. A base station according to any one of claims 37-40, **characterised in that** the base station (40) includes a means for transmitting also sensor (30) control data to the sensor (30) via the transmitter (43) of said link (33, 43).

42. A base station according to any one of claims 37-41, **characterised in that** its component transmitting energy to the sensor (30) is an inductive transmitter (43).

43. A base station according to any one of claims 37-42, **characterised in that** said component of the base station (40), receiving at least data, is a receiver (46) of a unidirectional and/or high-frequency RF link (36, 46).

44. A base station according to any one of claims 37-43, **characterised in that** the base station (40), or at least said component (43) functionally pertaining to it and transmitting energy, is arranged to be attached or is integrated with such support means or such construction pertaining to the imaging arrangement (50) which in connection with the imaging event is

positioned in the essential proximity, such as less than 50 cm, preferably less than 15 cm, such as to the distance of 2-8 cm, from the sensor (30) used in imaging, when the sensor is positioned in its imaging position, which construction is e.g. a headband or a collar or corresponding, the headrest of a dental chair, the X-ray source (4) used in imaging, or a part attachable to any of the abovementioned items.

45. A base station according to any of claims 37-44, **characterised in that** said transmitter (43) of the energy- transmitting link and/or receiver (46) of image data comprise a coil (34) and/or correspondingly an antenna (71), at least one of which is arranged to be attachable to the mouth- opening of the X-ray source (4) housing, or to the mouth- opening of a collimator tube (4') attachable to it, or to the immediate proximity of such mouth-opening, such as inside said mouth-opening.

46. A base station according to claim 45, **characterised in that** said transmitter (43) of the energy-transmitting link comprises a coil (34) which is essentially of the shape and size of the mouth-opening of said X-ray source (4) housing or of the collimator tube (4') attachable to it, or forms a part of an adapter (70) integrated, attached or arranged to be attachable in the essential proximity to said mouth-opening or to its essential proximity.

47. A base station according to any one of claims 37-46, **characterised in that** the electronics required for using said transmitter (43) of the energy-transmitting link and/or said receiver (46) of image data is integrated as part of the electronics of the X-ray source (4).

48. A base station according to any one of claims 37-47, **characterised in that** to the base station (40) is arranged a means for identifying those data packets possibly received which include damaged image data as well as a means for sending data regarding this to the sensor (30).

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Patentansprüche

1. Intraoralröntgenbildgebungsanordnung mit einem Steuersystem, einer Strahlungsquelle (4), die beispielsweise in Verbindung mit einer Gelenkarmkonstruktion (3) angeordnet ist, einem elektrischen Bilddatenempfänger (30), wie beispielsweise einem auf CMOS-Technologie beruhenden Sensor, und einer Drahtlosübertragungsverbindung (33, 43; 36, 46) zum Senden zumindest von durch den elektrischen Bilddatenempfänger (30) erfassten Bilddaten

- zu einer Basisstation (40) des elektrischen Bilddatenempfängers (30), zu einer Bildverarbeitungseinrichtung oder zu einer entsprechenden anderen Einrichtung, die Bildinformationen empfangen kann, wobei der Sender und der Empfänger der Übertragungsverbindung (33, 43; 36, 46) einerseits in Verbindung mit dem elektrischen Bilddatenempfänger (30) und andererseits zumindest in funktionsfähiger Verbindung mit der Basisstation (40) angeordnet sind,
- dadurch gekennzeichnet, dass** die Anordnung ferner eine Drahtlosleistungsübertragungsverbindung (33, 43) enthält, wobei diese Drahtlosleistungsübertragungsverbindung (33, 43) zur Verwendung zur Zufuhr von Energie zu dem elektrischen Bilddatenempfänger (30) in Verbindung mit einem Bildgebungsereignis eingerichtet ist.
2. Bildgebungsanordnung nach Anspruch 1, **dadurch gekennzeichnet, dass** ein Empfänger (33) der Leistungsübertragungsverbindung (33, 43) als Teil einer Elektronik des elektrischen Bilddatenempfängers angeordnet ist.
 3. Bildgebungsanordnung nach Anspruch 1 oder 2, **dadurch gekennzeichnet, dass** ein Empfänger (33) der Leistungsübertragungsverbindung (33, 43), der zur Elektronik des elektrischen Bilddatenempfängers gehört, die Primärleistungsquelle einer Leistungszufuhrschaltung (35), die zur Elektronik gehört.
 4. Bildgebungsanordnung nach einem der Ansprüche 1 bis 3, **dadurch gekennzeichnet, dass** der Empfänger (33) der Leistungsübertragungsverbindung (33, 43) eine Induktanz (33) oder ein HF-Empfänger (46) oder eine derartige entsprechende Komponente ist, die elektromagnetische Energie drahtlos aufnimmt, und die elektrisch nicht ladbar ist.
 5. Bildgebungsanordnung nach einem der Ansprüche 1 bis 4, **dadurch gekennzeichnet, dass** sie eine Einrichtung zum drahtlosen Übertragen von Energie zu dem elektrischen Bilddatenempfänger (30) während des tatsächlichen Bildgebungsereignisses enthält, die er in Verbindung mit einem Bildgebungsereignis benötigt.
 6. Bildgebungsanordnung nach einem der Ansprüche 1 bis 5, **dadurch gekennzeichnet, dass** die Gesamtenergiespeicherkapazität einer Komponente /von Komponenten, die eventuell zur Elektronik des elektrischen Bilddatenempfängers gehört/gehören, die Energie speichern können, geringer als die Energie ist, die durch den elektrischen Bilddatenempfänger (30) in Verbindung mit einem individuellen Bildgebungsereignis erforderlich ist.
 7. Bildgebungsanordnung nach einem der Ansprüche 1 bis 6, **dadurch gekennzeichnet, dass** die Gesamtenergiespeicherkapazität einer Komponente /von Komponenten, die eventuell zur Elektronik gehört/gehören, die Energie speichern können, weniger als 20 Ws, wie weniger als 5 Ws beträgt.
 8. Bildgebungsanordnung nach Anspruch 7, **dadurch gekennzeichnet, dass** die Gesamtenergiespeicherkapazität einer Komponente /von Komponenten, die eventuell zur Elektronik gehört/gehören, die Energie speichern können, weniger als 1-2 Ws beträgt.
 9. Bildgebungsanordnung nach einem der Ansprüche 1 bis 8, **dadurch gekennzeichnet, dass** der Arbeitsbereich der Leistungsübertragungsverbindung klein ist, wie unter 50 cm, vorzugsweise unter 15 cm, wie 2-8 cm.
 10. Bildgebungsanordnung nach einem der Ansprüche 1 bis 9, **dadurch gekennzeichnet, dass** der Sender (43) der Leistungsübertragungsverbindung (33, 43) an einem Ort oder einer Position platziert ist, oder zum Platzieren an einem Ort oder einer Position eingerichtet ist, an dem/der, wenn das abzubildende Objekt und der elektrische Bilddatenempfänger (30) gemäß der Bildgebungsanordnung (50) an ihren Abbildungspositionen positioniert sind, der elektrische Bilddatenempfänger (30) innerhalb des Arbeitsbereichs der Leistungsübertragungsverbindung (33, 43) positioniert ist.
 11. Bildgebungsanordnung nach Anspruch 10, **dadurch gekennzeichnet, dass** der Sender (4) der Leistungsübertragungsverbindung (33, 43) zum Platziertwerden an einer Strahlungsquelle (4) oder einer Basisstation (40), die in wesentlicher Verbindung mit dieser angeordnet ist, oder beispielsweise an einer Basisstation (40) eingerichtet ist, die an dem Patienten anbringbar oder an der Kopfstütze eines Zahnarztstuhls angeordnet ist.
 12. Bildgebungsanordnung nach einem der Ansprüche 1 bis 11, **dadurch gekennzeichnet, dass** sie eine Einrichtung zum Senden eines Signals von dem elektrischen Bilddatenempfänger (30) als Antwort auf den elektrischen Bilddatenempfänger (30) und den Sender (43) der Leistungsübertragungsverbindung (33, 43) enthält, die sich im Arbeitsbereich der Leistungsübertragungsverbindung (33, 43) befinden.
 13. Bildgebungsanordnung nach Anspruch 12, **dadurch gekennzeichnet, dass** sie eine Einrichtung zum Synchronisieren der Arbeitsweisen der Leistungsübertragungsverbindung (33, 43) und der Strahlungsquelle (4) enthält, sodass eine Abstrahlung nicht gestartet werden kann, wenn das Steuer-

- system der Bildgebungsanordnung (50) keine Informationen über den Empfänger (33) der Leistungsübertragungsverbindung (33, 43) hat, die an dem elektrischen Bilddatenempfänger (30) angeordnet ist, der sich im Arbeitsbereich der Leistungsübertragungsverbindung (33, 43) befindet.
14. Bildgebungsanordnung nach einem der Ansprüche 1 bis 13, **dadurch gekennzeichnet, dass** eine Einrichtung an dieser angeordnet ist, zur Steuerung der während eines Bildgebungsereignisses zu dem elektrischen Bilddatenempfänger (30) übertragenen Leistung und/oder der durch den elektrischen Bilddatenempfänger (30) während eines Bildgebungsereignisses verwendeten Leistung.
15. Bildgebungsanordnung nach einem der Ansprüche 1 bis 14, **dadurch gekennzeichnet, dass** die eine Einrichtung zur bidirektionalen Datenübertragung zwischen dem Empfänger von Bilddaten und dem Steuersystem der Bildgebungsanordnung (50) enthält, wobei die Daten zumindest Steuerbefehle und durch den Empfänger von Bilddaten erfasste Bilddaten umfassen.
16. Bildgebungsanordnung nach einem der Ansprüche 1 bis 15, **dadurch gekennzeichnet, dass** die Leistungsübertragungsverbindung (33, 43) zum Senden sowohl von vom elektrischen Bilddatenempfänger (30) benötigter Energie als auch von Steuersignalen des elektrischen Bilddatenempfängers (30) während des Bildgebungsereignisses eingerichtet ist.
17. Bildgebungsanordnung nach Anspruch 16, **dadurch gekennzeichnet, dass** die Leistungsübertragungsverbindung eine induktive Verbindung (33, 43) ist.
18. Bildgebungsanordnung nach Anspruch 17, **dadurch gekennzeichnet, dass** der Empfänger (33) der induktiven Verbindung (33, 43) eine Spule (34) umfasst, die im Wesentlichen die Form des elektrischen Bilddatenempfängers (30) -Umfangs nachahmt und sich zumindest teilweise in wesentlicher Nähe der Ränder des elektrischen Bilddatenempfängers befindet.
19. Bildgebungsanordnung nach Anspruch 17 oder 18, **dadurch gekennzeichnet, dass** eine oder mehrere relativ kleine Spulen am Empfänger von Bilddaten angeordnet sind, sodass sie sich beispielsweise in wesentlicher Nähe zu zumindest einer der Ecken des Empfängers von Bilddaten von im Wesentlichen rechteckiger Form befinden, wobei die Spule oder die Spulen zum Senden von Daten über die Position des Empfängers bezüglich des Senders (43) der induktiven Verbindung (33, 43) in dem durch sie erzeugten magnetischen Feld angeordnet sind.
20. Bildgebungsanordnung nach einem der Ansprüche 1 bis 19, **dadurch gekennzeichnet, dass** die Drahtlosübertragungsverbindung (36, 46) zum Senden zumindest der durch den elektrischen Bilddatenempfänger (30) erfassten Bilddaten eine HF-Verbindung ist.
21. Bildgebungsanordnung nach Anspruch 20, **dadurch gekennzeichnet, dass** die HF-Verbindung (36, 46) eine unidirektionale Verbindung ist und/oder eine Hochfrequenzverbindung ist und/oder Richtantennen mit ihr verwendet werden.
22. Elektrischer Drahtlosempfänger von Bilddaten, wie ein Sensor, insbesondere zur Verwendung in Verbindung mit einer Intraoralröntgenbildgebung, wobei der Empfänger ein Gehäuse und darin angeordnete Elektronik umfasst, die eine Erfassungseinrichtung (32) beispielsweise beruhend auf CMOS-Technologie, einen Sender zum Senden zumindest der durch die Erfassungseinrichtung (32) erfassten Bilddaten in den Äther und eine Leistungszufuhrschaltung (35) enthält, **dadurch gekennzeichnet, dass** die Leistungszufuhrschaltung ferner einen Empfänger (33) einer Drahtlosleistungsübertragungsverbindung (33, 43) enthält, wobei der Empfänger (33) eine Einrichtung enthält und/oder in funktionaler Verbindung mit diesem eine Einrichtung zum Empfangen und Senden von Energie in Verbindung mit einem Bildgebungsereignis angeordnet ist.
23. Elektrischer Drahtlosbilddatenempfänger nach Anspruch 22, **dadurch gekennzeichnet, dass** er eine Einrichtung zum Senden eines Signals von dem elektrischen Drahtlosbilddatenempfänger (30) als Antwort darauf enthält, dass er in den Arbeitsbereich der Leistungsübertragungsverbindung (33, 43) verbracht wird, wobei das Signal auch Identifizierungsdaten des in Frage kommenden elektrischen Drahtlosbilddatenempfängers umfassen kann.
24. Elektrischer Drahtlosbilddatenempfänger nach Anspruch 22 oder 23, **dadurch gekennzeichnet, dass** der Empfänger (33) der Leistungsübertragungsverbindung (33, 43) eine Induktanz oder ein HF-Empfänger oder eine derartige entsprechende Komponente ist, die elektromagnetische Energie drahtlos empfängt, und die elektrisch nicht ladbar ist.
25. Elektrischer Drahtlosbilddatenempfänger nach einem der Ansprüche 22 bis 24, **dadurch gekennzeichnet, dass** die Energiespeicherkapazität der eventuell zu der Leistungszufuhrschaltung (35) gehörenden Komponenten, die Energie speichern können, geringer als die durch den elektrischen Drahtlosbilddatenempfänger (30) in Verbindung mit einem individuellen Bildgebungsereignis erforderliche En-

- ergie ist.
26. Elektrischer Drahtlosbilddatenempfänger nach Anspruch 25, **dadurch gekennzeichnet, dass** die Gesamtenergiespeicherkapazität eines Kondensators /von Kondensatoren, der/die eventuell zur Elektronik gehört/gehören, die Energie speichern können, weniger als 20 Ws, wie weniger als 5 Ws beträgt. 5
27. Elektrischer Drahtlosbilddatenempfänger nach Anspruch 26, **dadurch gekennzeichnet, dass** die Gesamtenergiespeicherkapazität eines Kondensators /von Kondensatoren, der/die eventuell zur Elektronik gehört/gehören, die Energie speichern können, weniger als 1-2 Ws beträgt. 10
28. Elektrischer Drahtlosbilddatenempfänger nach einem der Ansprüche 22 bis 27, **dadurch gekennzeichnet, dass** eine Einrichtung an dem elektrischen Drahtlosbilddatenempfänger (30) zum Steuern der Leistung angeordnet ist, die er empfängt und/oder in Verbindung mit einem Bildgebungsereignis verbraucht. 20
29. Elektrischer Drahtlosbilddatenempfänger nach einem der Ansprüche 22 bis 28, **dadurch gekennzeichnet, dass** der Empfänger (33) der Leistungsübertragungsverbindung (33, 43) ein induktiver Empfänger (33) ist. 25
30. Elektrischer Drahtlosbilddatenempfänger nach Anspruch 29, **dadurch gekennzeichnet, dass** der Empfänger (33) der induktiven Verbindung (33, 43) eine Spule (34) umfasst, die im Wesentlichen die Form des elektrischen Drahtlosbilddatenempfänger (30)-Umfangs nachahmt und sich zumindest teilweise in wesentlicher Nähe der Ränder des elektrischen Drahtlosbilddatenempfängers befindet. 30
31. Elektrischer Drahtlosbilddatenempfänger nach Anspruch 30, **dadurch gekennzeichnet, dass** eine Einrichtung in funktionaler Verbindung mit der Spule (34) zum Messen und Senden von Informationen über die Stärke des durch den Sender (43) der induktiven Verbindung (33, 43) erzeugten Magnetfeldes angeordnet ist, der Leistung zu dem elektrischen Drahtlosbilddatenempfänger (30) überträgt. 40
32. Elektrischer Drahtlosbilddatenempfänger nach einem der Ansprüche 22 bis 31, **dadurch gekennzeichnet, dass** er ein Sensor (30) mit im Wesentlichen rechteckiger Form ist, wobei in wesentlicher Nähe zu zumindest einer Ecke dieses Rechtecks eine Spule angeordnet ist, mit der in funktionaler Verbindung eine Einrichtung zum Messen und Senden von Informationen über die Stärke des durch den Sender (43) der induktiven Verbindung (33, 43) erzeugten Magnetfeldes angeordnet ist, der Leistung zu dem Sensor (30) überträgt. 45
33. Elektrischer Drahtlosbilddatenempfänger nach einem der Ansprüche 22 bis 32, **dadurch gekennzeichnet, dass** die Elektronik eine Einrichtung zum Empfangen von Steuerdaten enthält, die eventuell in Verbindung mit der Drahtlosleistungsübertragung gesendet werden. 50
34. Elektrischer Drahtlosbilddatenempfänger nach einem der Ansprüche 22 bis 33, **dadurch gekennzeichnet, dass** seine Komponente, die Bilddaten überträgt, ein HF-Sender (36) ist, insbesondere ein Hochfrequenz-, wie 2,4 GHz, unidirektionaler HF-Sender (36) mit einer Richtantenne. 55
35. Elektrischer Drahtlosbilddatenempfänger nach einem der Ansprüche 22 bis 34, **dadurch gekennzeichnet, dass** die Elektronik eine Einrichtung zur gleichzeitigen Speicherung zumindest eines Teils der durch die Erfassungseinrichtung (32) erfassten Bilddaten in einem Speicher (38, 48), der zur Elektronik gehört, wie ein RAM oder ein Flash-Speicher, während immer noch Bilddaten erfasst werden, oder im Wesentlichen unmittelbar nach Beenden des Empfangs von Bilddaten enthält.
36. Elektrischer Drahtlosbilddatenempfänger nach Anspruch 35, **dadurch gekennzeichnet, dass** die Elektronik eine Einrichtung zur Neuübertragung der Bilddaten oder eines Teils der Bilddaten, die im Speicher (38, 48) gespeichert sind, als Antwort auf ein Steuersignal enthält, das durch den elektrischen Drahtlosbilddatenempfänger (30) drahtlos empfangen wird, wie den Empfänger (33) der bei der Leistungsübertragung verwendeten Verbindung (33, 43).
37. Basisstation für einen Intraoralröntgensensor, die Komponenten in funktionaler Verbindung miteinander umfasst, die eine elektronische Basisstation (40)-Anordnung bilden, wobei die Komponenten eine Komponente enthalten, die zumindest Bilddaten von einem bei einer Röntgenabbildung verwendeten Sensor (30) drahtlos empfängt, **dadurch gekennzeichnet, dass** die Basisstation ferner eine Einrichtung enthält, die zu dem Sensor (3) drahtlos Energie, die er in Verbindung mit einem Bildgebungsereignis braucht, als Antwort auf ein vom Sensor (30) in Verbindung mit dem Bildgebungsereignis empfangenes Signal überträgt, wobei entsprechend diesem Signal der Sensor (30) sich im Arbeitsbereich der Verbindung (33, 43) befindet.
38. Basisstation nach Anspruch 37, **dadurch gekennzeichnet, dass** das Signal derart aufgebaut ist, dass es vom Sensor (30) als Antwort auf ein durch den

Sensor (30) empfangenes Signal erhalten wird, das von der Basisstation (40) gesendet wird.

39. Basisstation nach Anspruch 38, **dadurch gekennzeichnet, dass** eine Einrichtung an der Basisstation (40) zum Verifizieren angeordnet ist, ob das Signal einen erkennbaren Identifizierer enthält, der den Sensor (30) identifiziert.
40. Basisstation nach einem der Ansprüche 37 bis 39, **dadurch gekennzeichnet, dass** die Elektronik der Basisstation (40) in funktionaler Verbindung mit einer Strahlungsquelle (4) angeordnet ist, die beim Abbilden verwendet wird, sodass die Verwendung der Strahlungsquelle (4) verhindert wird, wenn das Anordnungssteuersystem keine Daten über den bei der Abbildung verwendeten Sensor (30) hat, der sich im Arbeitsbereich der Verbindung (33, 43) befindet.
41. Basisstation nach einem der Ansprüche 37 bis 40, **dadurch gekennzeichnet, dass** die Basisstation (40) eine Einrichtung zum Senden von Sensor (30)-Steuerdaten zu dem Sensor (30) über den Sender (43) der Verbindung (33, 43) enthält.
42. Basisstation nach einem der Ansprüche 37 bis 41, **dadurch gekennzeichnet, dass** ihre Komponente, die Energie zum Sensor (30) überträgt, ein induktiver Sender (43) ist.
43. Basisstation nach einem der Ansprüche 37 bis 42, **dadurch gekennzeichnet, dass** die Komponente der Basisstation (40), die zumindest Daten empfängt, ein Empfänger (46) einer unidirektionalen und/oder Hochfrequenz-HF-Verbindung (36, 43) ist.
44. Basisstation nach einem der Ansprüche 37 bis 43, **dadurch gekennzeichnet, dass** die Basisstation (40) oder zumindest die Komponente (43), die funktional zu ihr gehört und Energie überträgt, zum Anbringen an oder integriert mit einer Hilfseinrichtung oder einem Aufbau eingerichtet ist, der zu der Bildgebungsanordnung (50) gehört, der in Verbindung mit dem Bildgebungsereignis in wesentlicher Nähe, wie weniger als 50 cm, vorzugsweise weniger als 15 cm, wie mit der Distanz von 2-8 cm vom bei der Abbildung verwendeten Sensor (30) positioniert ist, wenn der Sensor an seiner Abbildungsposition positioniert ist, wobei der Aufbau beispielsweise ein Stirrband oder ein Halsband oder Entsprechendes, die Kopfstütze eines Zahnarztstuhls, die bei der Abbildung verwendete Röntgenquelle (4) oder ein Teil ist, der an einem der vorstehenden Elemente anbringbar ist.
45. Basisstation nach einem der Ansprüche 37 bis 44, **dadurch gekennzeichnet, dass** der Sender (43) der Energie übertragenden Verbindung und/oder

der Empfänger (46) der Bilddaten eine Spule (34) und/oder entsprechend eine Antenne (71) umfasst, von denen zumindest ein Element an der Mundöffnung des Röntgenquellengehäuses oder der Mundöffnung einer Kollimatorröhre (4'), die an diesem anbringbar ist, oder in unmittelbarer Nähe der Mundöffnung, wie im Inneren der Mundöffnung anbringbar angeordnet ist.

46. Basisstation nach Anspruch 45, **dadurch gekennzeichnet, dass** der Sender (43) der Energie übertragenden Verbindung eine Spule (34) umfasst, die in Wesentlichen die Form und Größe der Mundöffnung des Gehäuses der Röntgenquelle (4) oder der daran anbringbaren Kollimatorröhre (4') aufweist, oder einen Teil eines Adapters (70) bildet, der in wesentlicher Nähe der Mundöffnung oder in ihrer wesentlichen Nähe integriert, angebracht oder anbringbar angeordnet ist.
47. Basisstation nach einem der Ansprüche 37 bis 46, **dadurch gekennzeichnet, dass** die zur Verwendung des Senders (43) der Energie übertragenden Verbindung und/oder des Empfängers (46) der Bilddaten erforderliche Elektronik als Teil der Elektronik der Röntgenquelle (4) integriert ist.
48. Basisstation nach einem der Ansprüche 37 bis 47, **dadurch gekennzeichnet, dass** an der Basisstation (40) eine Einrichtung zum Identifizieren solcher Datenpakete, die möglicherweise empfangen werden, die beschädigte Bilddaten enthalten, sowie eine Einrichtung zum Senden von Daten diesbezüglich zu dem Sensor (30) angeordnet sind.

Revendications

1. Agencement d'imagerie par rayons X intra-orale comprenant :
- un système de commande ;
 - une source de rayonnement (4) qui est agencée par exemple en relation avec une construction de bras articulé (3) ;
 - un récepteur de données d'image électrique (30) tel que par exemple un capteur basé sur la technologie CMOS ; et
 - une liaison de transmission sans fil (33, 43 ; 36, 46) pour transmettre au moins des données d'image détectées par le récepteur de données d'image électrique (30) à une station de base (40) du récepteur de données d'image électrique (30), à un dispositif de traitement d'image ou à un autre dispositif correspondant capable de recevoir des informations d'image, l'émetteur et le récepteur de la liaison de transmission (33, 43 ; 36, 46) sont agencés, d'une part, en relation

- avec le récepteur de données d'image électrique (30) et, d'autre part, au moins en relation fonctionnelle avec ladite station de base (40), **caractérisé en ce que** l'agencement comprend en outre une liaison de transmission de puissance sans fil (33, 43), laquelle liaison de transmission de puissance sans fil (33, 43) est agencée pour une utilisation pour alimenter le récepteur de données d'image électrique (30) avec une énergie en relation avec un événement d'imagerie.
2. Agencement d'imagerie selon la revendication 1, **caractérisé en ce qu'**un récepteur (33) de ladite liaison de transmission de puissance (33, 43) est agencé en tant que partie de l'électronique du récepteur de données d'image électrique.
 3. Agencement d'imagerie selon la revendication 1 ou 2, **caractérisé en ce qu'**un récepteur (33) de la liaison de transmission de puissance (33, 43) appartenant à l'électronique du récepteur de données d'image électrique est la source d'alimentation principale d'un circuit d'alimentation (35) appartenant à l'électronique.
 4. Agencement d'imagerie selon l'une quelconque des revendications 1 à 3, **caractérisé en ce que** le récepteur de la liaison de transmission de puissance (33, 43) est un récepteur inductif (33) ou un récepteur RF (46), ou un tel composant correspondant recevant une énergie électromagnétique par une liaison sans fil qui n'est pas chargeable électriquement.
 5. Agencement d'imagerie selon l'une quelconque des revendications 1 à 4, **caractérisé en ce qu'**il comprend des moyens pour transmettre, au récepteur de données d'image électrique (30), l'énergie dont il a besoin en relation avec un événement d'imagerie par une liaison sans fil pendant l'événement d'imagerie réel.
 6. Agencement d'imagerie selon l'une quelconque des revendications 1 à 5, **caractérisé en ce que** la capacité de stockage d'énergie totale du ou des composants appartenant éventuellement à l'électronique du récepteur de données d'image électrique qui sont capables de stocker l'énergie est inférieure à l'énergie nécessaire au récepteur de données d'image électrique (30) en relation avec un événement d'imagerie individuel.
 7. Agencement d'imagerie selon la revendication 6, **caractérisé en ce que** la capacité de stockage d'énergie totale du ou des composants appartenant éventuellement à l'électronique qui sont capables de stocker l'énergie est inférieure à 20 Ws, telle qu'inférieure à 5 Ws.
 8. Agencement d'imagerie selon la revendication 7, **caractérisé en ce que** la capacité de stockage d'énergie totale du ou des composants appartenant éventuellement à l'électronique qui sont capables de stocker l'énergie est inférieure à 1 à 2 Ws.
 9. Agencement d'imagerie selon l'une quelconque des revendications 1 à 8, **caractérisé en ce que** la plage de fonctionnement de ladite liaison de transmission de puissance (33, 43) est agencée pour être courte, telle qu'inférieure à 50 cm, de préférence inférieure à 15 cm, telle que de 2 à 8 cm.
 10. Agencement d'imagerie selon les revendications 1 à 9, **caractérisé en ce que** l'émetteur (43) de ladite liaison de transmission de puissance (33, 43) est placé ou agencé pour être placé à un emplacement ou à une position où, lorsque l'objet dont l'image doit être formée et ledit récepteur de données d'image électrique (30) sont positionnés à leurs positions d'imagerie conformément à l'agencement d'imagerie (50), le récepteur de données d'image électrique (30) est positionné dans la plage de fonctionnement de la liaison de transmission de puissance (33, 43).
 11. Agencement d'imagerie selon la revendication 10, **caractérisé en ce que** l'émetteur (4) de la liaison de transmission de puissance (33, 43) est agencé pour être placé sur une source de rayonnement (4) ou une station de base (40) agencée en relation essentielle avec celle-ci, ou par exemple une station de base (40) pouvant être fixée au patient ou agencée sur l'appui-tête d'un fauteuil de dentiste.
 12. Agencement d'imagerie selon l'une quelconque des revendications 1 à 11, **caractérisé en ce qu'**il comprend des moyens pour transmettre un signal à partir du récepteur de données d'image électrique (30) en réponse au fait que le récepteur de données d'image électrique (30) et l'émetteur (43) de la liaison de transmission de puissance (33, 43) sont situés dans la plage de fonctionnement de la liaison de transmission de puissance (33, 43).
 13. Agencement d'imagerie selon la revendication 12, **caractérisé en ce qu'**il comprend des moyens pour synchroniser les fonctionnements de ladite liaison de transmission de puissance (33, 43) et de la source de rayonnement (4) de sorte qu'un rayonnement ne puisse pas être débuté si le système de commande de l'agencement d'imagerie (50) ne dispose pas d'informations concernant le récepteur (33) de la liaison de transmission de puissance (33, 43) agencé sur le récepteur de données d'image électrique (30) situé dans la plage de fonctionnement de la liaison de transmission de puissance (33, 43).
 14. Agencement d'imagerie selon l'une quelconque des

- revendications 1 à 13, **caractérisé en ce que** des moyens ont été agencés sur celui-ci pour commander la puissance émise vers le récepteur de données d'image électrique (30) pendant un événement d'imagerie et/ou utilisée par le récepteur de données d'image électrique (30) pendant un événement d'imagerie.
15. Agencement d'imagerie selon l'une quelconque des revendications 1 à 14, **caractérisé en ce qu'**il comprend des moyens pour la transmission de données bidirectionnelle entre le récepteur de données d'image et le système de commande de l'agencement d'imagerie (50), lesquelles données comprennent au moins des commandes de contrôle et des données d'image détectées par le récepteur de données d'image.
16. Agencement d'imagerie selon l'une quelconque des revendications 1 à 15, **caractérisé en ce que** ladite liaison de transmission de puissance (33, 43) est agencée pour transmettre, pendant l'événement d'imagerie, à la fois l'énergie nécessaire au récepteur de données d'image électrique (30) et les signaux de commande du récepteur de données d'image électrique (30).
17. Agencement d'imagerie selon la revendication 16, **caractérisé en ce que** ladite liaison de transmission de puissance est une liaison inductive (33, 43).
18. Agencement d'imagerie selon la revendication 17, **caractérisé en ce que** le récepteur (33) de ladite liaison inductive (33, 43) comprend une bobine (34) imitant essentiellement la forme du périmètre du récepteur de données d'image électrique (30) et qui est située au moins en partie dans le voisinage essentiel des bords du récepteur de données d'image électrique.
19. Agencement d'imagerie selon la revendication 17 ou 18, **caractérisé en ce qu'**une ou plusieurs bobines relativement petites sont agencées sur ledit récepteur de données d'image de sorte qu'elles soient situées, par exemple, à proximité essentielle d'au moins l'un des coins du récepteur de données d'image de forme essentiellement rectangulaire, laquelle bobine ou lesquelles bobines sont agencées pour transmettre des données concernant la position dudit récepteur par rapport à l'émetteur (43) de ladite liaison inductive (33, 43) dans le champ magnétique produit par celui-ci.
20. Agencement d'imagerie selon l'une quelconque des revendications 1 à 19, **caractérisé en ce que** ladite liaison de transmission sans fil (36, 46) pour transmettre au moins les données d'image détectées par le récepteur de données d'image électrique (30) est
- une liaison RF.
21. Agencement d'imagerie selon la revendication 20, **caractérisé en ce que** ladite liaison RF (36, 46) est une liaison unidirectionnelle et/ou une liaison haute fréquence et/ou des antennes directionnelles sont utilisées dans celle-ci.
22. Récepteur de données d'image électrique sans fil, tel qu'un capteur, particulièrement pour une utilisation en relation avec une imagerie par rayons X introrale, lequel récepteur comprend un logement et une électronique agencée dans celui-ci, laquelle électronique comprend un détecteur (32) basé par exemple sur la technologie CMOS, un émetteur pour transmettre au moins les données d'image détectées par ledit détecteur (32) sur les ondes et un circuit d'alimentation (35), **caractérisé en ce que** le circuit d'alimentation comprend en outre un récepteur (33) d'une liaison de transmission de puissance sans fil (33, 43), lequel récepteur (33) comprend et/ou en relation fonctionnelle avec lequel sont agencés des moyens pour recevoir et transmettre l'énergie en relation avec un événement d'imagerie.
23. Récepteur de données d'image électrique sans fil selon la revendication 22, **caractérisé en ce qu'**il comprend des moyens pour transmettre un signal à partir du récepteur de données d'image électrique sans fil (30) en réponse au fait qu'il est amené dans la plage de fonctionnement de ladite liaison de transmission de puissance (33, 43), lequel signal peut également comprendre des données d'identification du récepteur de données d'image électrique sans fil en question.
24. Récepteur de données d'image électrique sans fil selon la revendication 22 ou 23, **caractérisé en ce que** ledit récepteur (33) de la liaison de transmission de puissance (33, 43) est un récepteur inductif ou un récepteur RF, ou un tel composant correspondant recevant l'énergie électromagnétique par une liaison sans fil, qui n'est pas chargeable électriquement.
25. Récepteur de données d'image électrique sans fil selon l'une quelconque des revendications 22 à 24, **caractérisé en ce que** la capacité de stockage d'énergie des composants appartenant éventuellement au circuit d'alimentation (35) qui sont capables de stocker l'énergie est inférieure à l'énergie nécessaire au récepteur de données d'image électrique sans fil (30) en relation avec un événement d'imagerie individuel.
26. Récepteur de données d'image électrique sans fil selon la revendication 25, **caractérisé en ce que** la capacité de stockage d'énergie totale du ou des con-

- densateurs appartenant éventuellement à l'électronique qui sont capables de stocker l'énergie est inférieure à 20 Ws, telle qu'inférieure à 5 Ws.
27. Récepteur de données d'image électrique sans fil selon la revendication 26, **caractérisé en ce que** la capacité de stockage d'énergie totale du ou des condensateurs appartenant éventuellement à l'électronique est inférieure à 1 à 2 Ws.
28. Récepteur de données d'image électrique sans fil selon l'une quelconque des revendications 22 à 27, **caractérisé en ce que** des moyens ont été agencés sur le récepteur de données d'image électrique sans fil (30) pour commander la puissance qu'il reçoit et/ou utilise en relation avec un événement d'imagerie.
29. Récepteur de données d'image électrique sans fil selon l'une quelconque des revendications 22 à 28, **caractérisé en ce que** ledit récepteur (33) de la liaison de transmission de puissance (33, 43) est un récepteur inductif (33).
30. Récepteur de données d'image électrique sans fil selon la revendication 29, **caractérisé en ce que** ledit récepteur (33) de la liaison inductive (33, 43) comprend une bobine (34) imitant essentiellement la forme du périmètre du récepteur de données d'image électrique sans fil (30) et qui est située au moins en partie dans le voisinage essentiel des bords du récepteur de données d'image électrique sans fil.
31. Récepteur de données d'image électrique sans fil selon la revendication 30, **caractérisé en ce que** des moyens ont été agencés en relation fonctionnelle avec ladite bobine (34) pour mesurer et transmettre des informations concernant l'intensité du champ magnétique formé par l'émetteur (43) de la liaison inductive (33, 43) qui transmet la puissance au récepteur de données d'image électrique sans fil (30).
32. Récepteur de données d'image électrique sans fil selon l'une quelconque des revendications 22 à 31, **caractérisé en ce qu'il s'agit d'un capteur (30)** de forme essentiellement rectangulaire, à proximité essentielle d'au moins un coin duquel rectangle une bobine est agencée, en relation fonctionnelle avec lequel des moyens sont agencés pour mesurer et transmettre des informations concernant l'intensité du champ magnétique formé par l'émetteur (43) de la liaison inductive (33, 43) qui transmet la puissance au capteur (30).
33. Récepteur de données d'image électrique sans fil selon l'une quelconque des revendications 22 à 32, **caractérisé en ce que** l'électronique comprend des moyens pour recevoir des données de commande transmises éventuellement en relation avec ladite transmission de puissance sans fil.
34. Récepteur de données d'image électrique sans fil selon l'une quelconque des revendications 22 à 33, **caractérisé en ce que** le composant de celui-ci transmettant des données d'image est un émetteur RF (36), particulièrement un émetteur haute fréquence, tel qu'un émetteur RF unidirectionnel à 2,4 GHz (36) comprenant une antenne directionnelle.
35. Récepteur de données d'image électrique sans fil selon l'une quelconque des revendications 22 à 34, **caractérisé en ce que** l'électronique comprend des moyens pour mémoriser au moins une partie des données d'image détectées par le détecteur (32) dans une mémoire (38, 48) appartenant à l'électronique, telle qu'une mémoire vive ou une mémoire flash, simultanément alors que les données d'image sont encore détectées ou essentiellement immédiatement à la fin de la réception des données d'image.
36. Récepteur de données d'image électrique sans fil selon la revendication 35, **caractérisé en ce que** l'électronique comprend des moyens pour retransmettre les données d'image, ou une partie de celles-ci, mémorisées dans ladite mémoire (38, 48), en réponse à un signal de commande qui est reçu par le récepteur de données d'image électrique sans fil (30) par une liaison sans fil, par exemple par l'intermédiaire dudit récepteur (33) de la liaison (33, 43) utilisée pour la transmission de puissance.
37. Station de base pour un capteur de rayons X introral, qui comprend des composants en relation fonctionnelle les uns avec les autres formant un agencement électronique de station de base (40), lesquels composants comprennent un composant recevant, par une liaison sans fil, au moins des données d'image d'un capteur (30) utilisé dans une imagerie par rayons X, **caractérisée en ce que** la station de base (40) comprend en outre des moyens pour transmettre, par une liaison sans fil, au capteur (3), l'énergie dont il a besoin en relation avec un événement d'imagerie, en réponse à un signal reçu dudit capteur (30) en relation avec l'événement d'imagerie, conformément auquel signal, le capteur (30) est situé dans la plage de fonctionnement de ladite liaison (33, 43).
38. Station de base selon la revendication 37, **caractérisée en ce que** ledit signal est agencé pour être atteint à partir du capteur (30) en réponse à un signal reçu par le capteur (30) qui est envoyé par la station de base (40).

39. Station de base selon la revendication 38, **caractérisée en ce que** des moyens sont agencés sur la station de base (40) pour vérifier si ledit signal comprend un identifiant reconnaissable, qui identifiera le capteur (30). 5
40. Station de base selon l'une quelconque des revendications 37 à 39, **caractérisée en ce que** l'électronique de la station de base (40) est agencée en relation fonctionnelle avec une source de rayonnement (4) utilisée pour l'imagerie de sorte que l'utilisation de la source de rayonnement (4) sera empêchée si le système de commande d'agencement ne dispose pas de données concernant ledit capteur (30) utilisé pour l'imagerie qui est situé dans ladite plage de fonctionnement de la liaison (33, 43). 10
41. Station de base selon l'une quelconque des revendications 37 à 40, **caractérisée en ce que** la station de base (40) comprend des moyens pour transmettre également des données de commande du capteur (30) au capteur (30) par l'intermédiaire de l'émetteur (43) de ladite liaison (33, 43). 15
42. Station de base selon l'une quelconque des revendications 37 à 41, **caractérisée en ce que** son composant transmettant l'énergie au capteur (30) est un émetteur inductif (43). 20
43. Station de base selon l'une quelconque des revendications 37 à 42, **caractérisée en ce que** ledit composant de la station de base (40), recevant au moins des données, est un récepteur (46) d'une liaison RF unidirectionnelle et/ou haute fréquence (36, 46). 25
44. Station de base selon l'une quelconque des revendications 37 à 43, **caractérisée en ce que** la station de base (40), ou au moins ledit composant (43) appartenant fonctionnellement à celle-ci et transmettant l'énergie, est agencée pour être attachée ou est intégrée avec de tels moyens de support ou une telle construction appartenant à l'agencement d'imagerie (50) qui est positionné en relation avec l'événement d'imagerie à proximité essentielle, par exemple à moins de 50 cm, de préférence à moins de 15 cm, par exemple à la distance de 2 à 8 cm, du capteur (30) utilisé pour l'imagerie, lorsque le capteur est positionné à sa position d'imagerie, laquelle construction est par exemple un bandeau ou un collier ou un élément correspondant, l'appuie-tête d'un fauteuil de dentiste, la source de rayons X (4) utilisée pour l'imagerie, ou une pièce pouvant être fixée à l'un quelconque des éléments mentionnés ci-dessus. 30
45. Station de base selon l'une quelconque des revendications 37 à 44, **caractérisée en ce que** ledit émetteur (43) de la liaison de transmission d'énergie et/ou le récepteur (46) de données d'image comprennent 35
- une bobine (34) et/ou de manière correspondante une antenne (71), au moins l'une de celles-ci est agencée pour pouvoir être fixée à l'ouverture d'entrée du logement de la source de rayons X (4), ou à l'ouverture d'entrée d'un tube de collimation (4') pouvant être fixé à celle-ci, ou à proximité immédiate de cette ouverture d'entrée, par exemple à l'intérieur de ladite ouverture d'entrée. 40
46. Station de base selon la revendication 45, **caractérisée en ce que** ledit émetteur (43) de la liaison de transmission d'énergie comprend une bobine (34) qui est essentiellement de la forme et de la taille de l'ouverture d'entrée dudit logement de la source de rayons X (4) ou du tube de collimation (4') pouvant être fixé à celle-ci, forme une partie d'un adaptateur (70) intégré, attaché ou agencé pour pouvoir être fixé à proximité essentielle de ladite ouverture d'entrée ou à sa proximité essentielle. 45
47. Station de base selon l'une quelconque des revendications 37 à 46, **caractérisée en ce que** l'électronique nécessaire pour utiliser ledit émetteur (43) de la liaison de transmission d'énergie et/ou ledit récepteur (46) de données d'image est intégrée en tant que partie de l'électronique de la source de rayons X (4). 50
48. Station de base selon l'une quelconque des revendications 37 à 47, **caractérisée en ce que** des moyens sont agencés sur la station de base (40) pour identifier les paquets de données éventuellement reçus qui comprennent des données d'image endommagées, ainsi que des moyens pour envoyer des données concernant celles-ci au capteur (30). 55

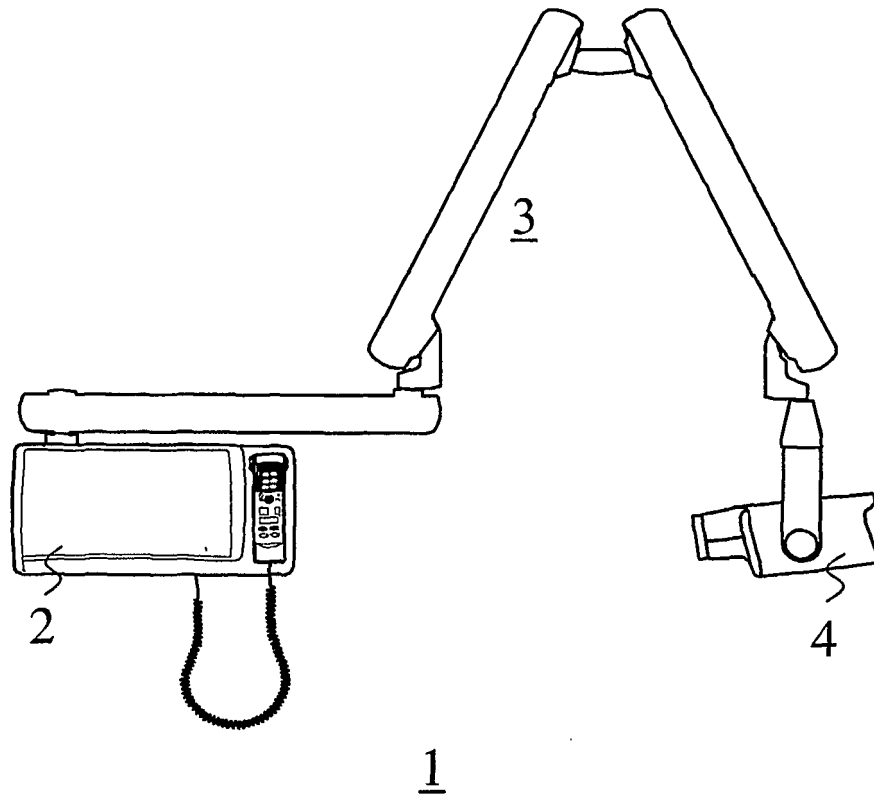
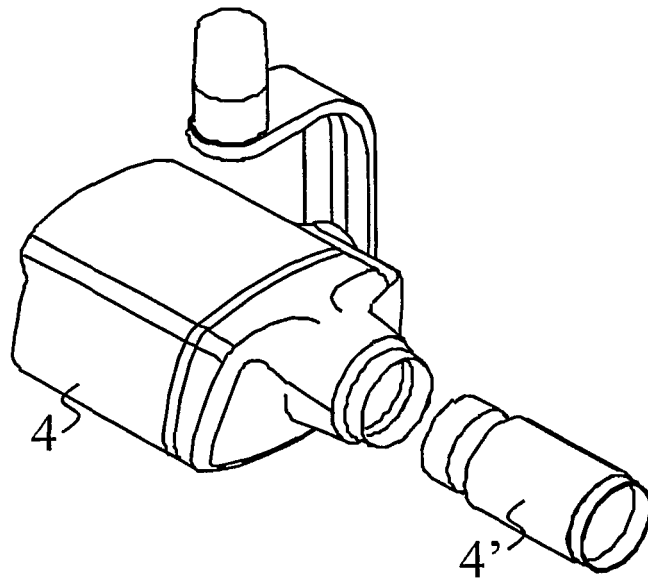
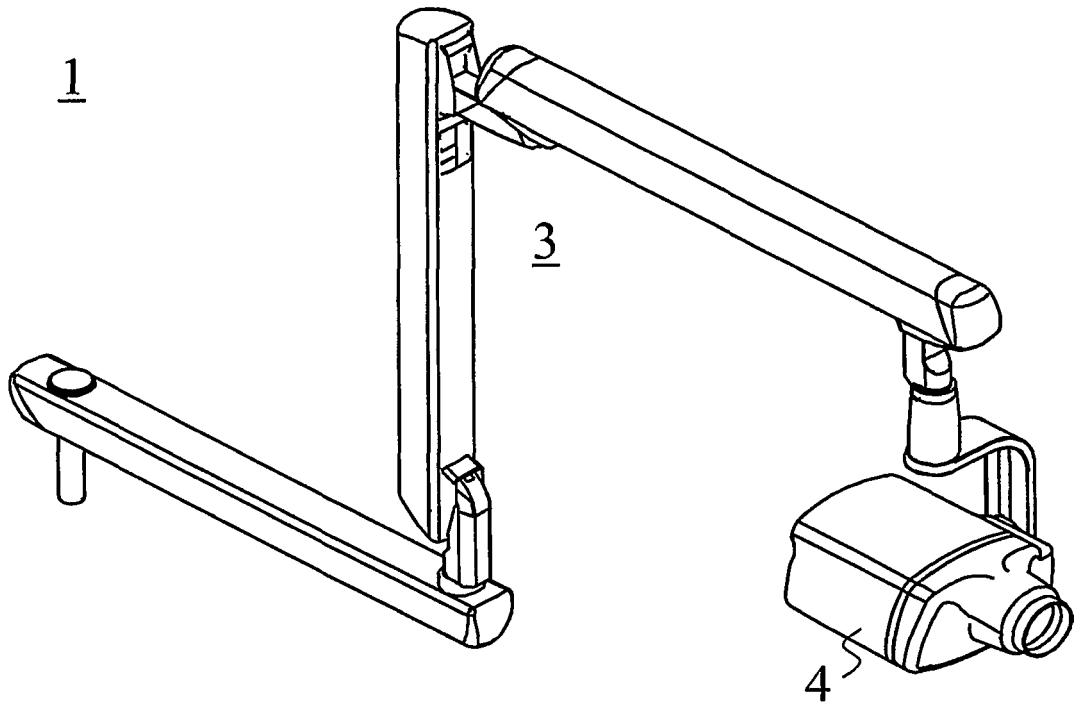


Fig. 1



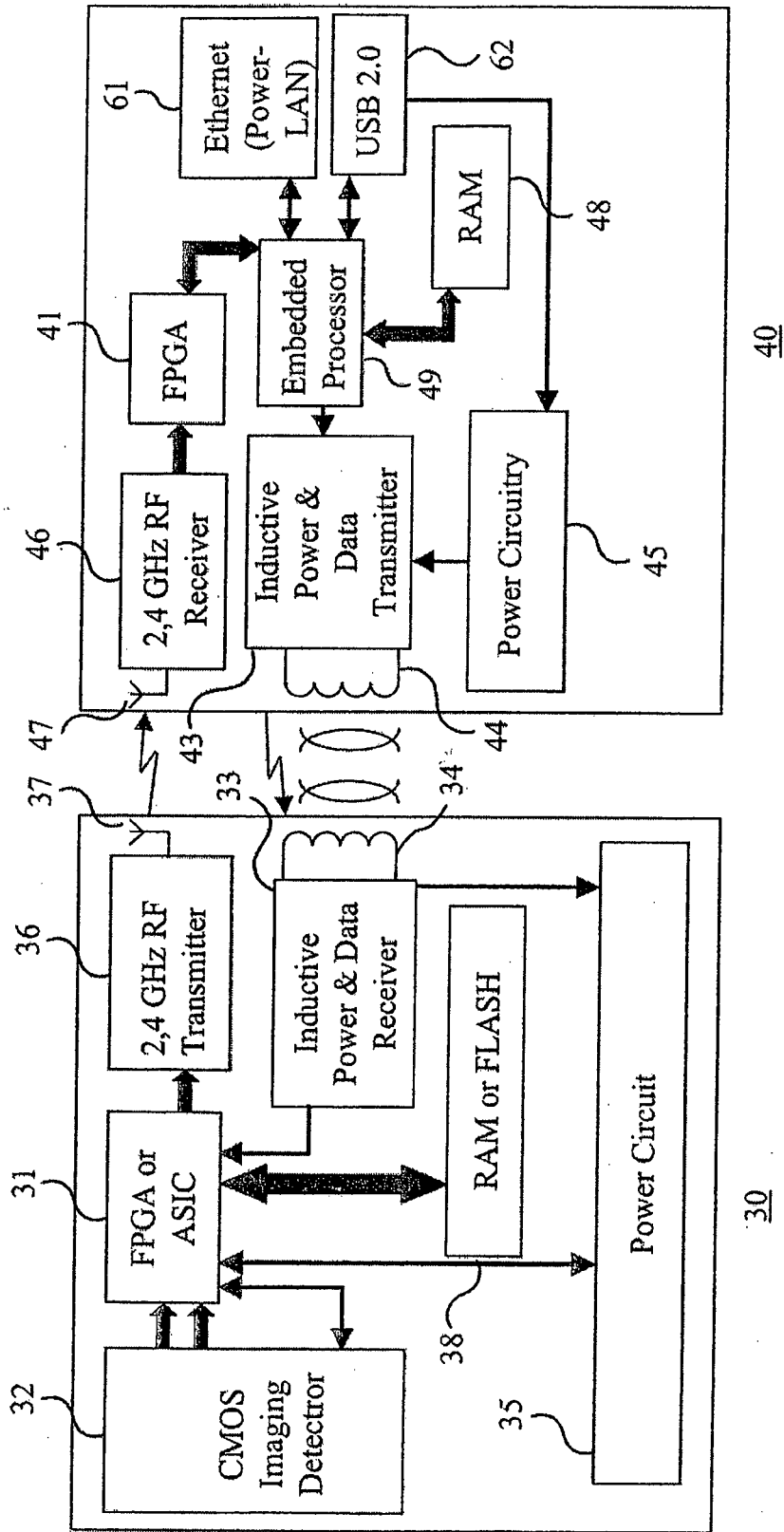


Fig. 3

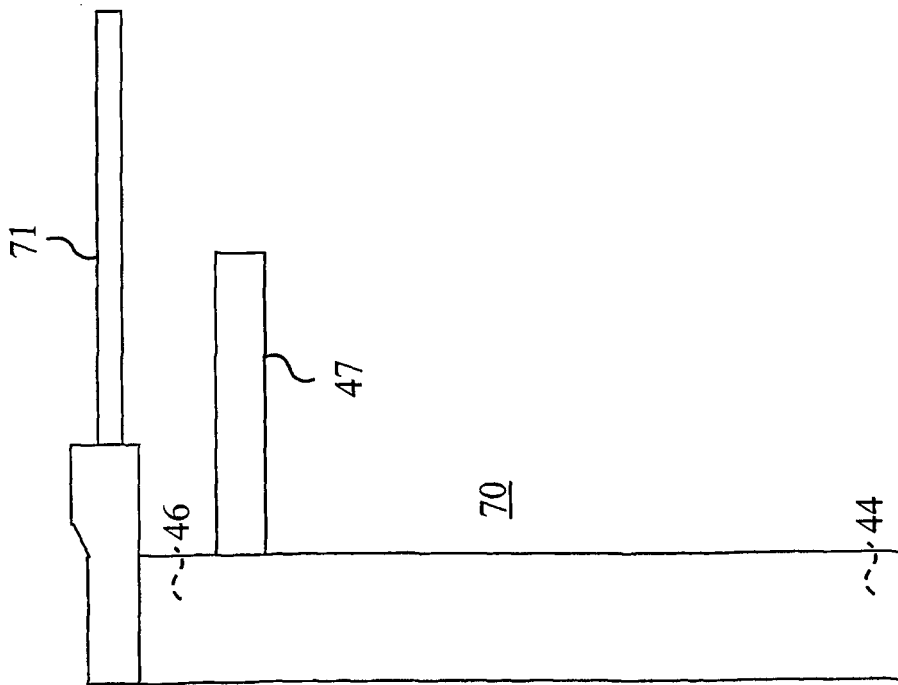


Fig. 4a

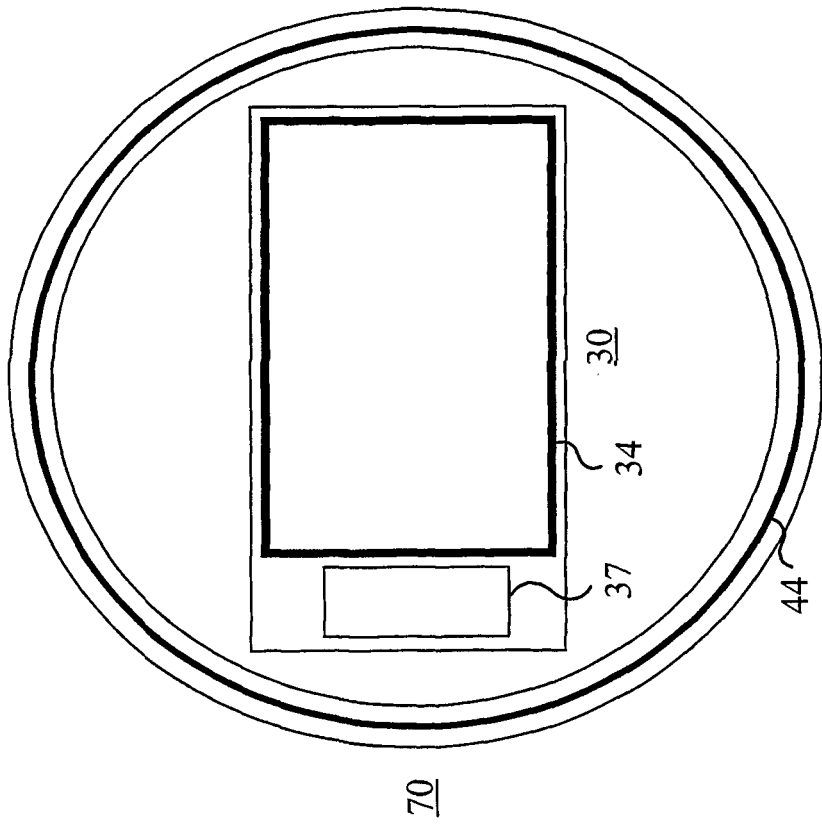


Fig. 4b

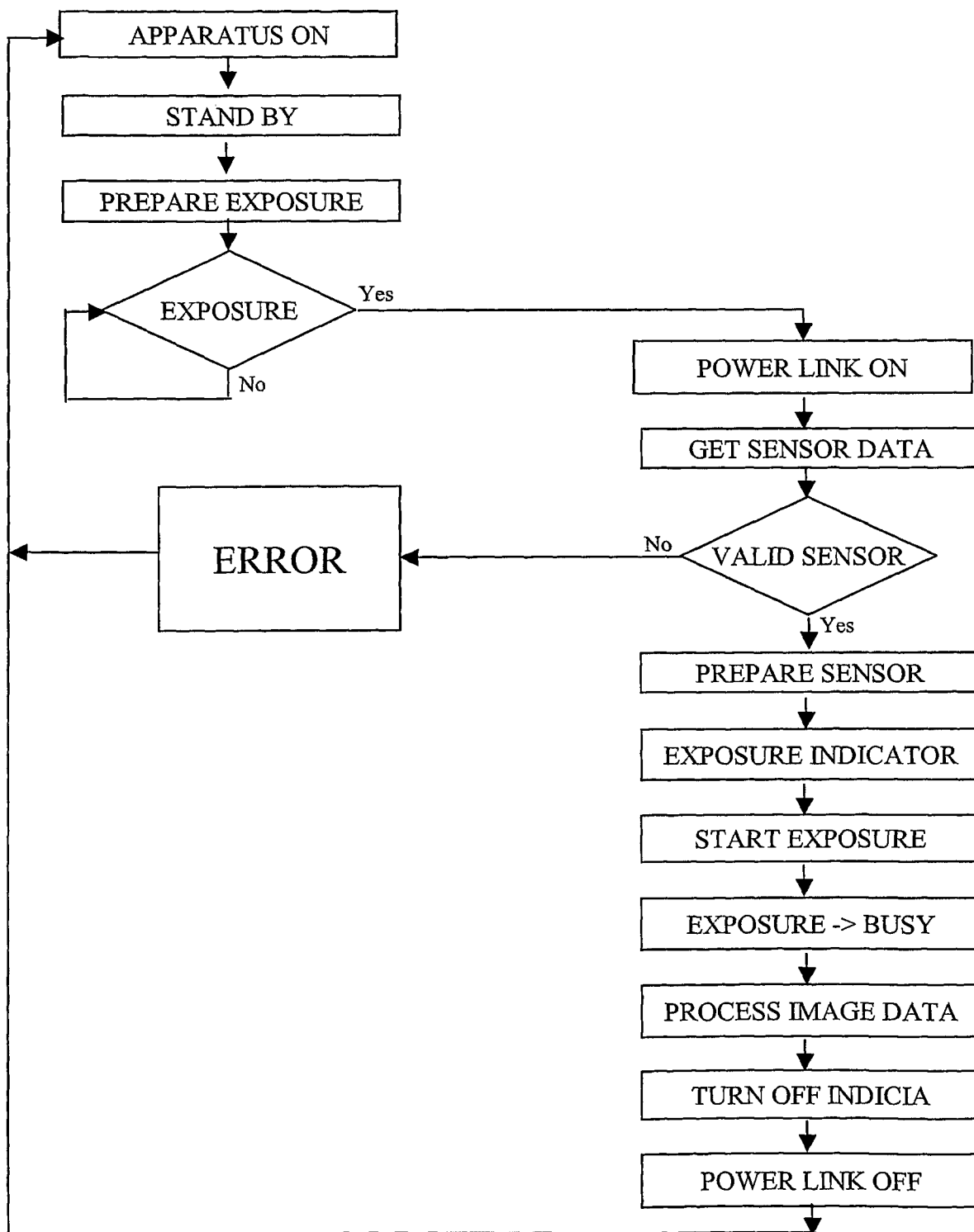


Fig. 5

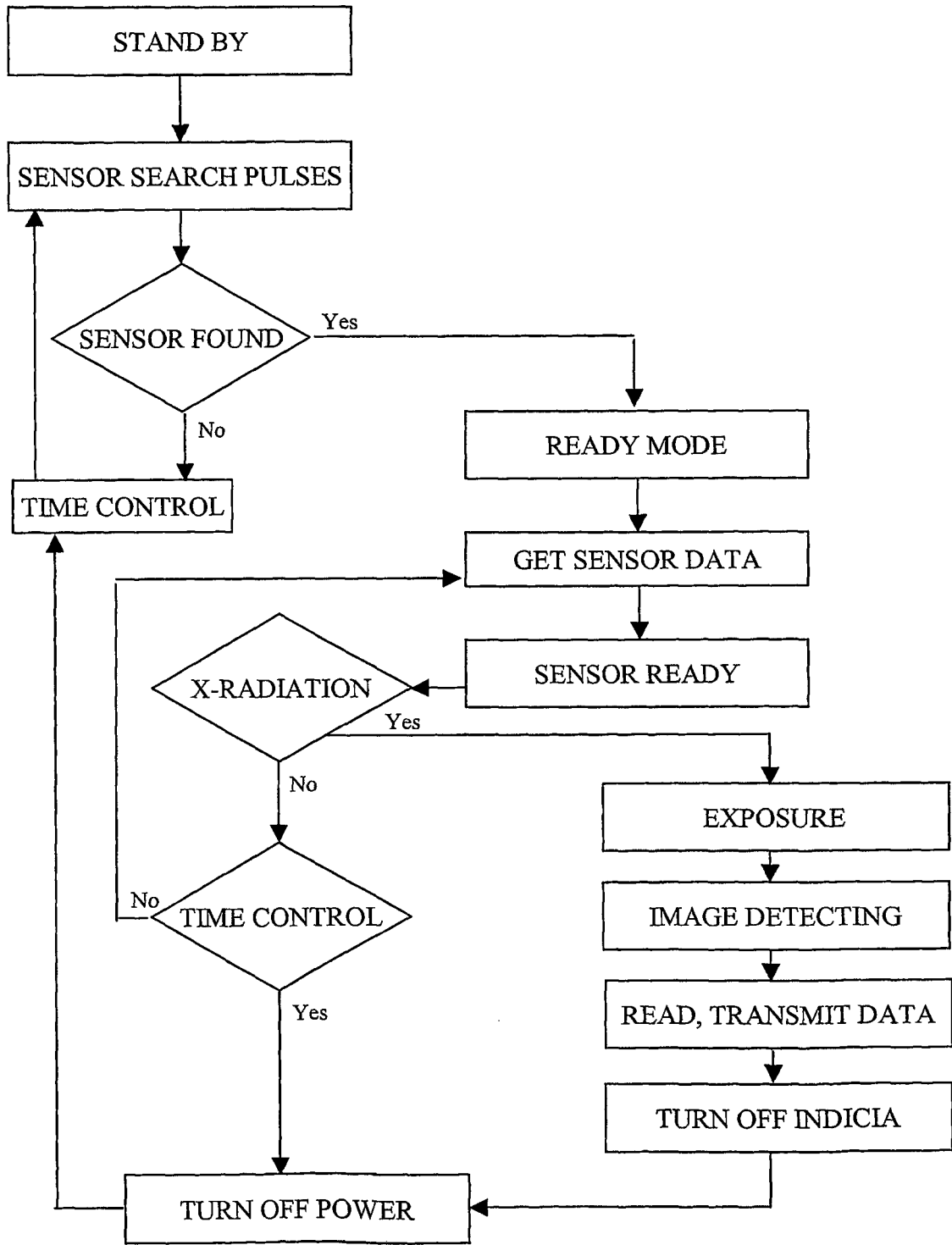


Fig. 6

REFERENCES CITED IN THE DESCRIPTION

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专利名称(译)	无线口内X射线成像		
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摘要(译)

本发明涉及x射线成像，尤其涉及用于口内x射线成像的成像装置，无线成像传感器和用于传感器的基站，以及用于向传感器提供操作功率的方法。无线地将信息传输到传感器和传感器，在本发明中使用这样的无线电力传输链路，其被布置成用于与成像过程一起向传感器供应能量。