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(54) **Sensor system comprising an integrated optical waveguide for the detection of chemical substances**

(57) The sensor system for the detection of chemical substances has an optical waveguide (6) which produces an evanescent field penetrating into the adjacent medium (7), a light source (2) for coupling light into the waveguide (6), and a detecting circuit (9) for receiving light from the waveguide (6) and producing an output

signal (11) reflecting the sensed chemical substance. In the preferred embodiment, the waveguide has the form of a bifilar, non-crossing spiral. It consists of an incoming or decreasing spiral segment (12) and an outgoing or increasing spiral segment (13) continuously bound by a pair of opposite central semi-circular segments (14).

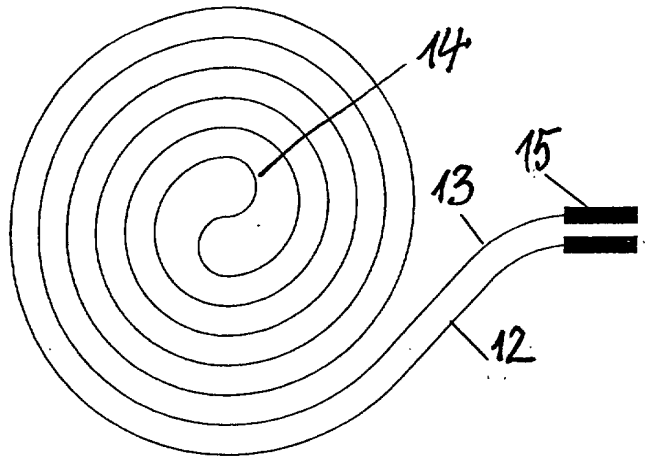


Fig. 3

EP 1 291 642 A1

Description

5 [0001] The present invention concerns a sensor system for the detection of chemical substances in an adjacent medium, by spectral analysis, with an optical waveguide adapted to produce an evanescent field for penetrating into the adjacent medium and interacting with it, light source means for coupling light into the waveguide, and detector means for receiving light from the waveguide and producing an output signal reflecting the sensed chemical substance.

10 [0002] The general aim of the present invention is the detection of gas or liquid concentrations, especially in the presence of a gas or liquid mixture. More particularly, the present invention is directed to the field of gas permeation, mainly in the medical field where transcutaneous blood gases are to be detected, e.g. carbon dioxide, oxygen and possibly anaesthetic gases within the blood. Such gases permeate through the patient skin at very low flow rate.

15 [0003] According to the most well-known detection methods the interaction between the light and the detected medium usually occurs in a free-space cell which can be a single-or a multi-pass cell depending on whether the cell facets are reflecting light or not. Most of the systems make use of an optical cell through which the analyte is flowing and in which the whole light beam interacts with the medium molecules. In the last decades systems using fiber optic evanescent field detection have been proved but interaction length and reliability are the main limitations of such systems for industrial application.

20 [0004] It is also well known that integrated waveguides can be applied as chemical sensors using evanescent field interaction. Thus reference may be made to Lambeck, P.V. in "Sensors and actuators B ", vol.8, 1992, p. 103-116, where mainly two properties of the detected medium, spectral absorption and refractive index which are combined in a complex dielectric constant, interact within the evanescent field on an integrated optical waveguide.

25 [0005] Further reference may be made to Pandraud, G. et al. in "Sensors and actuators B ", Chemical 85, 2000, p. 158-162 where evanescent wave sensing is described with an accent on optical absorption of the detected medium applying the Lambert-Beer law as read-out principle and micro-fluidic direct bonding for sampling cell miniaturization. The resulting cell volume is about $200 \mu\text{m} \cdot 400 \mu\text{m} \cdot 1\text{cm} = 0.8 \text{mm}^3$ and is well adapted to micro-fluidic analysis.

30 [0006] But as mentioned before, the present invention generally aims at detecting chemicals in very small volumes or permeating through membranes. In the case of transcutaneous blood gas detection the gas permeates through the patient skin at flow rates of approximately $1 \mu\text{l} \cdot \text{cm}^{-2} \cdot \text{min}^{-1}$. With such flow rates a volume of 0.8mm^3 over a $400 \mu\text{m} \cdot 1 \text{cm}$ surface would rise the response time to 20 min which is two orders of magnitude too high for transcutaneous gas detection.

35 [0007] As a possible solution of this problem it has been considered to increase the interaction length but especially within a small sensing surface in the order of one square centimeter.

40 [0008] In the prior art specific waveguide curvatures and geometries performing high packing density have been proposed: WO 9400750 shows two waveguide geometries performing dense interaction length per unit area, one in a zigzag shape and one in a spiral shape. The principle uses spectral analysis, at the output, of an injected coded bundle or light pulse. The proposed zigzag waveguide exhibits a clear disadvantage as the waveguide occupation fraction rises when the zigzag curvature becomes strong. The limit is reached as the curvature losses become critical but this limit is reached for each zigzag leading to strong total losses as the waveguide occupation fraction is optimized. The proposed spiral waveguide is characterized by a relative short distance between two adjacent segment inducing voluntary cross-coupling. In addition the central ends of the enlaced spiral do not form a continuous waveguide.

45 [0009] A spiral shape detector is also shown in US Patent No. 5394239. The goal of the patent is to integrate on a chip an interferometric sensor. It is constituted by a double enlaced spiral waveguide with crossings of all individual windings to get out from the center of the spiral. The crossings consist of a bridge requiring multiple masks so that the process time/cost is relatively high.

50 [0010] In GB 2 222 881 a detection principle is described which is a continuous signal (DC) detection using strong resonant waveguide, the spectrum of which is adjusted to match the line spacing of the absorption of the detected medium. In this case the sensitivity is enhanced by using a light source spectral width significantly larger than the absorption line width of the detected medium, ideally covering many absorption lines. Moreover the active stabilization of the resonance wavelength is required to maintain a good match of the resonance wavelength to the source wavelength if various lines of the detected gas. Moreover, a continuous signal detection (DC) in spectroscopy, which is sensitive to the absorption baseline fluctuations, is much more noisy than the detection of a modulated signal (AC) used in so-called "modulation spectroscopy" which, on the contrary, guarantees a perfect absorption baseline rejection.

55 [0011] In view of the above the present invention has the object of providing a sensor system which is free from the disadvantages of the known sensor systems.

[0012] According to the invention high packing densities and sensitivities are achieved by a sensor system in which the waveguide has the form of a bifilar, non-crossing spiral consisting of an incoming or decreasing spiral segment and an outgoing or increasing spiral segment continuously bound by a pair of opposite central semi-circular segment.

[0013] For the purpose of this specification the term bifilar is used in the basic meaning of involving a single thread doubled back upon itself. The term is not supposed to include a configuration with threads twisted about each other.

[0014] Aside from the use in the medical field, especially for transcutaneous blood gas measurement the sensor system according to the invention is applicable in the fields of gas analysis, monitoring of gas production and in micro-structure processing, automotive, environmental and food industries etc.

[0015] The fact that sensors according to the present invention are constituted by non-crossing waveguides reduces the number of masks needed for processing to a minimum. The detection principle does not use interference signals so that the chemical refractive index variation exhibited by chemical mixtures, does not influence the measurement signal. In the particular case of detection by spectral analysis in the mid-infrared range (overtone detection), the signal delivered by the sensor may be very low and sensitive spectroscopic techniques may be used in conjunction with evanescent sensing.

[0016] According to a preferred embodiment of the invention a wavelength modulation spectroscopy technique is used which provides a rejection of the absorption baseline fluctuations leading to an enhanced molecule selectivity and sensitivity in chemical mixture.

[0017] In the following a preferred embodiment of the invention is described with regard to the accompanying drawings in which

Fig. 1 shows a schematic diagram of a sensor system

Fig. 2 shows a cross-section of the sensor portion

Fig. 3 shows a typical geometry of a sensor waveguide

Fig. 4 shows an alternative waveguide geometry

Fig. 5 shows a diagram of the resonant cavity signal enhancement

Fig. 6 A shows a resonance grid scan

Fig. 6 B shows a scan diagram of modulation parameters

[0018] The sensor system shown in Fig. 1 uses an integrated optical waveguide for evanescent wave sensing of the surrounding medium and in a preferred embodiment a technique of wavelength modulation for spectroscopy. A signal generator 1 is connected to a light source 2 whereby the so-called signal generator effects a wavelength modulation as described in the following general equation for sine modulation:

$$I_{opt} \propto E \cdot E^* \quad \text{and} \quad E_{LD}(t) \propto \sqrt{1 + M \cdot \cos(2\pi \cdot \nu_m \cdot t + \varphi)} \cdot e^{i\left(2\pi \cdot \nu_0 \cdot t + \frac{\Delta \nu_m}{\nu_m} \cdot \sin(2\pi \cdot \nu_m \cdot t)\right)}$$

where I_{opt} and E are respectively the optical intensity and the optical complex electric-field generated by the light source 2, M is the intensity modulation index, ν_m is the modulation frequency, t the time, φ the phase-lag between intensity modulation and optical frequency modulation, $\Delta \nu_m$ represents the optical frequency-modulation amplitude corresponding to the excursion of the optical frequency around the central optical frequency ν_0 .

[0019] The light source 2, which delivers an optical signal to fiber 3, is modulated both in wavelength and intensity according to the working principle of the current modulated semiconductor laser diode. The amplitude modulation is eliminated by taking the difference of the measured signal delivered by fiber 8 and the reference signal delivered by fiber 10 to the opto-electronic detection circuit. A balanced detection delivers an output signal 8, which is analyzed in its first and second Fourier components, corresponding to the fundamental and first harmonic signals. Either the fundamental term or the first harmonic term or a combination of both may be used to quantify the intensity of the absorption line of the medium.

[0020] The light source 2 is connected via an optical fiber 3 to a fiber coupler or optical power splitter 4 splitting the light beam into two output beams guided by two output fibers. A first output fiber 5 is coupled to the input of an integrated optics waveguide 6. This is effected by gluing or welding the corresponding optical fiber 5 into an integrated V-groove of the integrated optics circuit 6. The fiber optical field is adapted, using an integrated taper or a mode converter, to the waveguide propagation mode reducing the overall transmission losses and optical reflections at the waveguide ends. The waveguide ends possibly generate interferometric noise.

[0021] Interferometric noise will be understood in this description as having the following origin: The interferometric noise results from time fluctuations of the detected signal. These fluctuations, which may appear as random, periodical or pseudo-periodical, result from the interference(s) of the multiply reflected and transmitted optical waves propagating

in the optical circuitry. These reflections originate from the undesired changes of the refractive indexes and of the waveguide geometry along the optical path and from the connectors in the optical circuit. Optical cavities may result from these discontinuities, typically at the fluid cell facets (the waveguide ends in our case) and at the optical component interfaces. Periodical or pseudo-periodical resonances, which are sensitive to the cavity length L_{cav} and refractive index n_{cav} variations, appear and modulate the spectrum of the optical signal. The resonance period is called cavity free-spectral-range FSR and is defined as:

$$FSR = \frac{c}{2 n_{cav} L_{cav}}$$

where c is the vacuum speed of light.

[0022] Hence, any changes in cavity length or refractive index will vary the cavity FSR which causes a shift of the q -th resonance of the cavity. The q -th resonance satisfies the following equation:

$$q \lambda = 2 n_{cav} L_{cav}$$

where λ is the optical wavelength of the light propagation throughout the cavity.

Consequently either a shift of the cavity spectrum or a wavelength change of the optical wave, as created in wavelength modulation spectroscopy, produces time fluctuations of the output signal called "interferometric noise".

[0023] The whole optical circuit has been designed in order to minimize the interferometric noise of the exciting and collecting fiber by elongating these fibers in such a way that the interferometric noise associated to these fibers can be eliminated by high frequency rejection and averaging. The most important part of the interferometric noise originate from the measurement waveguide itself, forming a cavity with resonances interfering severely with the gas spectral lines. The measurement waveguide length may be varied mainly by temperature and the waveguide effective refractive index may be influenced by the detected medium refractive index. The latter can undergo deep variations in the presence of gas mixture.

[0024] The amplitude of the interferometric noise is influenced by the optical reflections at the interfaces and discontinuities along the optical path. In particular, the sensing cavity formed by the integrated optics waveguide 6 is a source of interferometric noise which degrades the signal from the medium. Reducing the reflections at the waveguide ends contributes to reduce determinedly the interferometric noise.

[0025] Many types of light sources having a bandwidth narrower than the absorption lines of the analyzed medium can be used. Laser diodes, solid state lasers and fiber lasers are convenient. In a preferred embodiment, a DFB laser diode, stabilized in DC-current and temperature, is used as light source 2. The signal generator 1 is used to drive the current of the DFB diode. A modulation of the wavelength results from the current modulation. A ramp or sine or the superposition of both is generated by the signal generator resulting in a wavelength which is sinusoidally modulated around a central wavelength that can be ramped.

[0026] In some cases, the spectral lines, characteristic of different substances or different isotopes of the same substance, have wavelengths which are close enough to be scanned individually by ramping the wavelength of the light source over a sufficient spectral interval. The concentration of several substances or their isotopes can be determined simultaneously. In other cases, where the spectral lines are too far in the spectrum, several light sources can be used sequentially.

[0027] In the particular case of a sensor working in the near- or mid-infrared spectral range, the waveguide 6 is produced using (but not restricted to) the known Si₃N₄/SiO₂ technology on Si-substrate. The Si₃N₄/SiO₂/Si high guidance technology has been optimized for evanescent wave sensitivity and propagation loss. It allows strong waveguide curvature leading to a very long spiral length (can be easily raised to 1m length) on a typical 1 cm diameter substrate area.

[0028] The question of the choice of the optimal length of the measurement waveguide cannot be solved generally. It results from a compromise between the needed interaction length and the severity of the losses which increases with length and attenuate the signal. So an optimal waveguide length can be found, which is a function of the propagation losses generally expressed in dB/cm. Using the present technology developments the optimal waveguide length has been found to be 14.5cm for -0.3dB/cm propagation loss.

[0029] At each end the waveguide 6 is provided with a V-groove for so-called fiber pigtailling (i.e. setting the position and helping for gluing or welding) and a taper or a mode converter (see fig. 2). It performs the coupling and the transition from the optical fiber mode to the integrated waveguide mode. Moreover the waveguide ends can be angled for interferometric noise reduction (typical angles are in the order of 8°)

[0030] The output fiber 8 of the waveguide 6 is coupled to a first input of a balanced opto-electronic detection circuit

9. The second output fiber 10 of coupler 4 is directly coupled to a second input of the detection circuit 9.

[0031] The modulated light coming from the light source is split in coupler 4 into a measurement signal which is fed to the waveguide and a reference signal. The power of the reference signal may be adjusted by introducing a fibered optical attenuator (not shown). Both the reference signal and the output signal from the waveguide are compared

5 according to a balanced detection principle in the electronic detection circuit 9.

[0032] The resulting signal at output 11 of the detection circuit represents the concentration of the gas/liquid detected in the medium 7 because the evanescent wave of the uncovered integrated waveguide 8 interacts within the medium 7.

[0033] The waveguide schematically shown in Fig. 3 is composed of an incoming segment 12 and an outgoing segment 13 bound continuously by a pair of opposite semi-circular segment 14. By this configuration a non-crossing spiral waveguide is formed. The distance between two adjacent segments is large enough to prevent cross-coupling. At the ends of the waveguide an integrated taper or mode converter 15 is implemented to improve coupling efficiency and to reduce the interferometric noise. As already mentioned, an integrated V-groove is implemented to ease the positioning and the gluing/welding of the corresponding optical fibers.

[0034] Fig. 4 presents the sketch of several waveguides interlaced in such a way that no crossing and no cross-coupling occur. Such a configuration can be used to sense several substances in parallel when it is connected to several light sources and several detectors.

[0035] In order to enhance the system signal-to-noise ratio (SNR) two different methods are appropriate which concern the wavelength modulation technique (by the signal generator (1)) of the light source (2), by the adjustment of the parameters of the signal generator.

20 One by tuning parameters on the waveguide resonance spectrum in order to enhance the signal and the other by tuning the parameters for interferometric noise rejection. For both methods the light source spectral width is narrow compared to the absorption line width of the selected medium.

[0036] The first method is based on the adjustment of the modulation frequency: the modulation frequency of the light source is made equal to a fraction or a multiple of the free-spectral-range (FSR) of the dominant cavity. The elimination of most of the refractive index steps along the optical path by a careful design of the optical circuit has the consequence that the measurement waveguide, for which the interfaces between the waveguide and the optical fibers (or waveguide ends) constitutes the dominant optical cavity, having resonances contributing strongly to the generation of the interferometric noise. The modulation frequency will be chosen according to the following formula:

$$v_m = \text{FSR} \cdot k \quad (k = \dots, 1/3, 1/2, 1, 2, 3\dots)$$

30 wherein v_m corresponds to the wavelength modulation frequency in Hz and FSR is the optical cavity free-spectral-range in Hz.

[0037] Preferably, the cavity length is equal to the waveguide length (chosen for optimal sensitivity) and the cavity refractive index corresponds to the waveguide effective refractive index (in the order of around 1.6). With this choice of the modulating frequency, the resonant cavity performs as a spectral filter providing the signal enhancement. The Fig. 5 illustrates the particular case of $v_m = \text{FSR}$.

[0038] The modulated light source input signal spectrum (1), consisting of Dirac's peaks, is matched to the resonant cavity spectrum (2) through its modulation frequency ν_m which has been adjusted to be equal to the free-spectral-range FSR of the cavity. This adjustment is independent of the gas/liquid absorption line/spectrum (3). The only requirement is that the resonant cavity FSR must be smaller than the absorption line width allowing frequency-modulation amplitude Δv_m to be optimized for maximal sensitivity. The optimal frequency-modulation amplitude Δv_m is in the same order of magnitude as the absorption line width (full-width at half-maximum).

[0039] This method is applied in the case of stable or stabilized cavity free-spectral-range which can be controlled through temperature for example. This method apply preferably strong resonant cavity for signal enhancement but optimal signal-to-noise ratio corresponds to the compromise between signal enhancement and system stability.

[0040] In the case of strongly varying cavity characteristics the first method is not applicable anymore and interferometric noise will be generated by the measurement cavity. Such a situation will occur, for example, when gas mixtures or temperature are unpredictable. It is often the case in transcutaneous blood gas detection.

[0041] An alternate method (Second method) involves two steps, where the modulation parameters comprising at least the modulation frequency and the frequency-modulation amplitude are determined in order to achieve strong interferometric noise rejection.

[0042] The first two parameters, modulation frequency and frequency-modulation amplitude, of the light source are set to initial values, called ideal values, defined as the values of the parameters which offer the maximal sensitivity to gas/liquid spectral characteristics, in the particular case where no interferometric noise is generated. These ideal values for the parameters are determined for each characteristic gas/liquid absorption spectral line.

In a second step, the case where a non negligible interferometric noise is generated by the measurement cavity, is

addressed. An optimization procedure is performed: the initial values of the parameters are modified in a continuous way, in order to reach new values, called optimal values, defined as the values of the parameters which minimize the interferometric noise, while keeping the highest sensitivity to the spectral lines of the gas / liquid species.

[0043] As a consequence of this procedure, perturbation of the signal induced by the variation of the waveguide length and/or effective refractive index can be minimized by the use of the optimized values of the modulation parameters. The latter result must be considered as a major achievement of the patent, because the determination of the optimal values of the modulation parameters also provides a large insensitivity of the concentration to the refractive index of the analyzed medium.

[0044] In a preferred embodiment the preferred waveguide length, which has been chosen for optimal sensitivity, is 14.5cm and the refractive index 1.6 (not restricted to these values). The elimination of most of the irregularities along the optical path by a careful design of the optical circuit has been achieved and the measurement cavity formed by the measuring waveguide constitutes the dominant optical cavity, generating resonances characterized by a free-spectral-range (FSR) of 0.646GHz, measured at the output system by sweeping the optical frequency of the light source 2 under stabilized cavity spectrum. Additional sweep of the frequency-modulation amplitude around ideal parameters set gives rise to a two-dimensional grid of resonances illustrated by the simulation results shown in Fig. 6 A. The bold black lines represent optimal situations in both optical frequency shift and frequency-modulation amplitude axis. As the interferometric noise originates from a random shift of the resonances along the optical frequency axis the interferometric noise can be estimated as the standard deviation over the optical frequency range.

[0045] To illustrate this second method, Fig.6 B illustrates typical two-dimensional scan of the modulation frequency and frequency-modulation amplitude.

[0046] It is a particular merit of the present invention that it could be demonstrated that for some particular values of the modulation frequency and the modulation-frequency amplitude the signal could be made insensitive to the shift of the optical frequencies or, in another interpretation, insensitive to the variation of the FSR and/or the length of the dominant cavity.

[0047] In the particular situation corresponding to the preferred embodiment, optimal situation takes place where noise (mainly from interferometric origin) is minimal. The dependence on the frequency-modulation amplitude is strong but weak on the modulation frequency. So the optimal parameters sets appears all along the bottom of the "valleys" giving more freedom on the modulation frequency choice.

In the preferred embodiment the modulation frequency is fixed to 200MHz for electronic convenience without any restriction, then the optimal modulation amplitude is tuned at 4.85GHz (as shown in Fig. 6 B) which is the nearest value around the ideal parameters set which modulation amplitude was 4.9 GHz.

[0048] Finally the optimal parameters set reached through the second method confers to the whole system an interferometric noise rejection so that system sensitivity can be considered as almost independent regarding to detected medium refractive index variations or waveguide length variations.

[0049] In summary, in addition to high selectivity and absorption baseline rejection due to modulation spectroscopy the achievements yielded by the second method are

- a) high sensitivity due to optimal parameters set near the ideal parameters set
- b) high interferometric noise rejection due to the determination of optimal parameters set
- c) high signal-to-noise ratio (SNR) due to a) and b)
- d) high independence towards waveguide length and effective refractive index variations due to b)
- e) high independence towards detected medium refractive index variations due to d).

[0050] Considering all these advantages, the second method can be considered as an important innovation in gas/liquid sensing, especially in the absorption spectroscopy field and is applied to the preferred embodiment of the present invention.

Claims

1. Sensor system for the detection of chemical substances in an adjacent medium, with an integrated optical waveguide adapted to produce an evanescent field for penetrating into the adjacent medium, light source means for coupling light into the waveguide, and detector means for receiving light from the waveguide and producing an output signal reflecting the sensed chemical substance.
2. A sensor system according to claim 1, **characterized by** the fact that the waveguide has the form of a bifilar, non-crossing spiral consisting of an incoming or decreasing spiral segment and an outgoing or increasing spiral segment continuously bound by a pair of opposite central semi-circular segment.

3. A sensor system according to claim 2, **characterized by** the fact that the detector means comprise an opto-electronic detection circuit producing an output signal reflecting the sensed chemical substance.
- 5 4. A sensor system according to claim 2, **characterized by** an optical power splitter located between the light source and the waveguide for feeding an optical signal to the incoming segment of the waveguide and an optical reference signal.
- 10 5. A sensor system according to claim 4, **characterized in that** an optical output signal from the outgoing segment of the waveguide is fed together with the reference signal to the detector for balanced detection.
- 15 6. A sensor system according to one of the preceding claims, **characterized by** the fact that the waveguide is constituted by a multiplicity of individual spiral waveguides enlaced together forming a multiple non-crossing, cross-coupling-free spiral waveguide, whereby each individual waveguide associated with a different wavelength.
- 20 7. A sensor system according to one of claims 1-5, **characterized by** the fact that the light source is wavelength-modulated and the detection circuitry is adapted for fundamental and/or harmonics detection.
- 25 8. A sensor system where the input and output fibers are elongated in such a way that the interferometric noise generated by these fibers can be eliminated.
- 30 9. A method for the detection of chemical substances in an adjacent medium using a system according to one of the preceding claims, **characterized in that** at least the wavelength modulation frequency is determined in order to achieve signal enhancement. The wavelength modulation frequency is adapted to the free-spectral-range (FSR) of the optical cavity generating the most relevant resonance spectrum according to the formula $\nu_m = k \cdot \text{FSR}$ ($k = \dots, 1/3, 1/2, 1, 2, 3\dots$), wherein ν_m corresponds to the wavelength modulation frequency in Hz and FSR is the optical cavity free-spectral-range in Hz and wherein FSR depends on the cavity length and effective refractive index as modeled by the equation $\text{FSR} = c / 2 \cdot N_{\text{cav}} \cdot L_{\text{cav}}$ for a typical cavity, wherein c is the vacuum speed of light and N_{cav} , L_{cav} are the effective refractive index and the geometrical length of the cavity respectively.
- 35 10. A method for the detection of chemical substances in an adjacent medium using a system according to claim 8 where the FSR of the dominant cavity is kept constant by the control of the temperature of the cavity.
- 40 11. A method for the detection of chemical substances in an adjacent medium using a system according to one of the preceding claims, **characterized in that** at least the modulation frequency and the frequency-modulation amplitude, called modulation parameters, are determined in order to achieve strong interferometric noise rejection. The method is comprises three steps, the first step is to fix the modulation parameters at their ideal values corresponding to the case of no interferometric noise, the second step is to perform a multi-dimensional scan of the modulation parameters around the ideal parameters values while measuring the noise level of the whole sensor system, the third step is to adjust the modulation parameters to the nearest values around the ideal values but where the noise level of the whole sensor system is significantly lower.
- 45 12. A sensor system for the detection of chemical substances in an adjacent medium using any one or a combination of the preceding claims, where several substances can be sensed by scanning sequentially several wavelengths.
- 50 13. A sensor system for the detection of chemical substances in an adjacent medium using any one or a combination of the preceding claims, where several substances can be sensed by different non-crossing optical waveguides interlaced on the same substrate.
- 55 14. A sensor system for the detection of chemical substances in an adjacent medium using any one or a combination of the preceding claims, where several substances can be sensed by using several light sources in a sequence or in parallel.

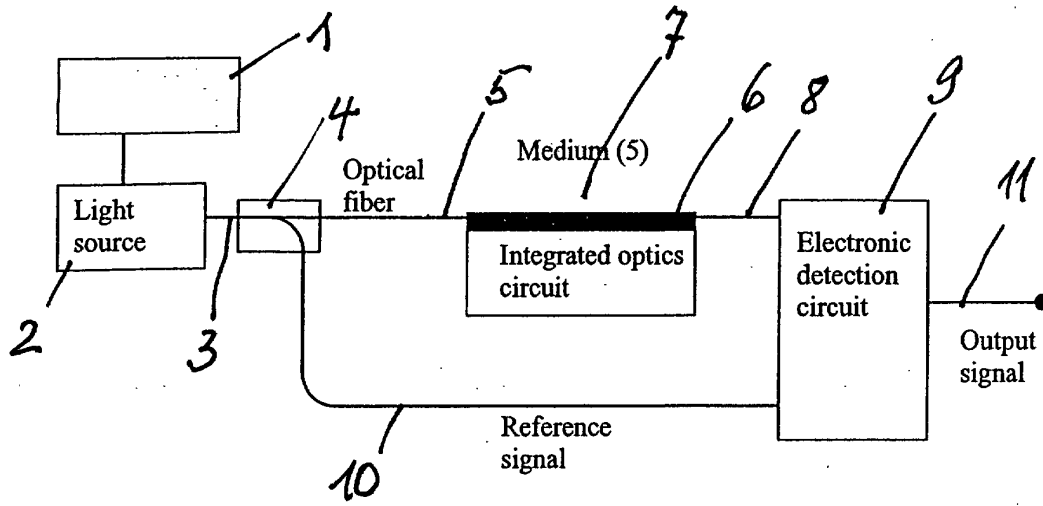


Fig. 1

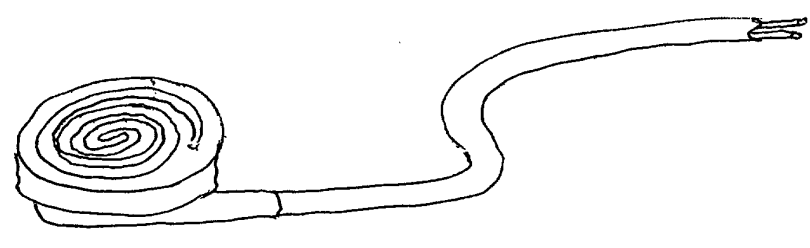


Fig. 2

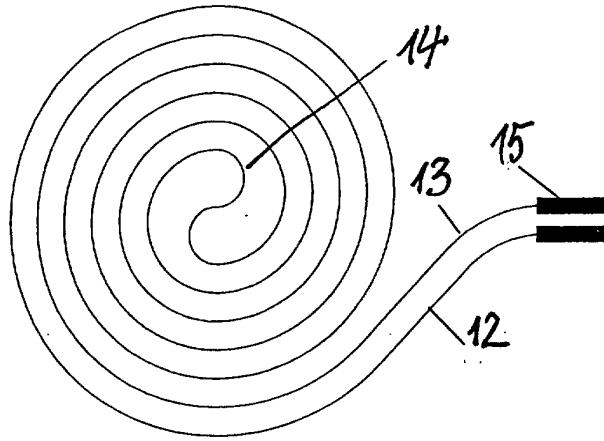


Fig. 3

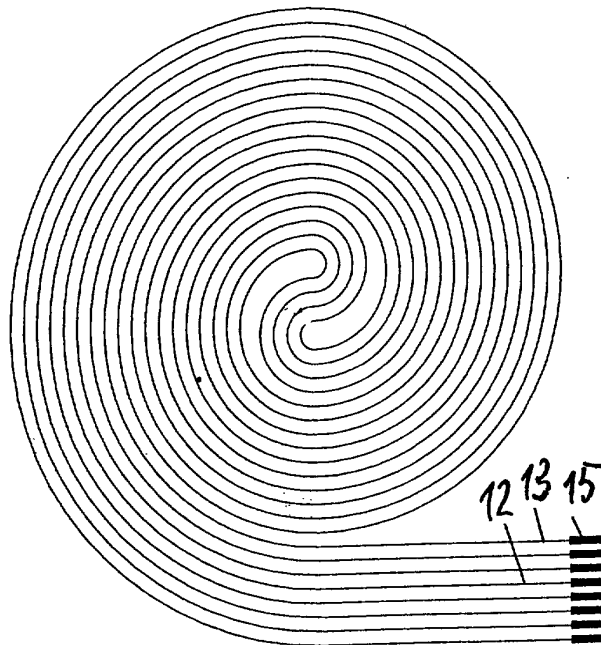


Fig. 4

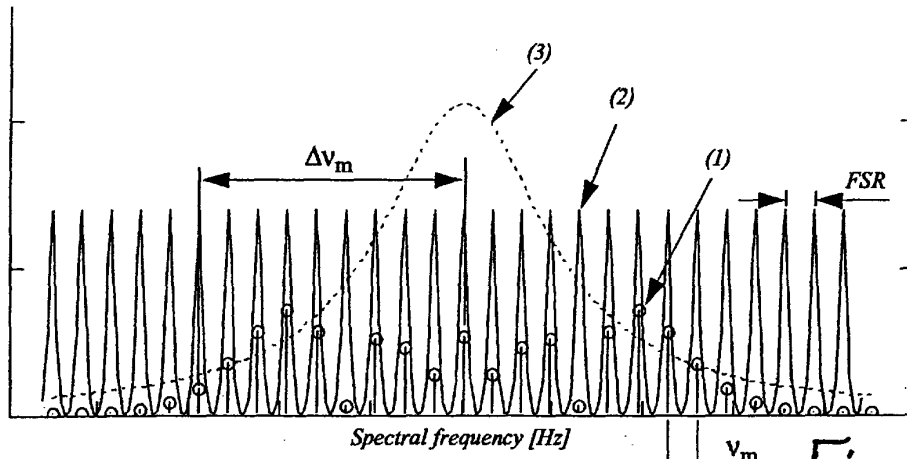


Fig. 5

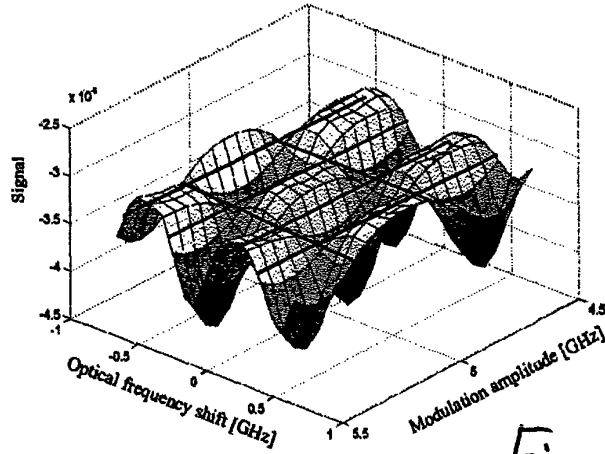


Fig. 6A

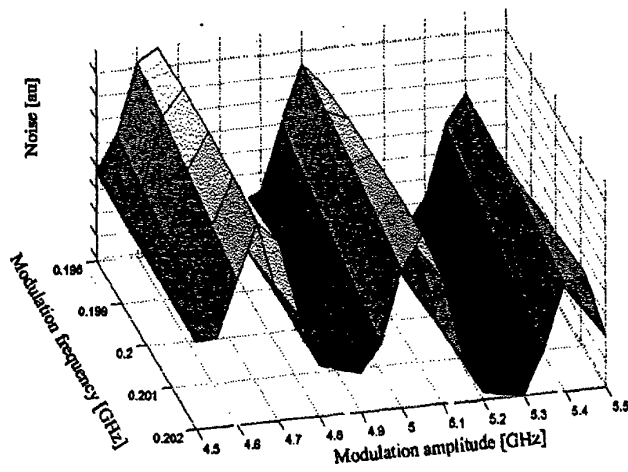


Fig. 6B



European Patent
Office

EUROPEAN SEARCH REPORT

Application Number
EP 01 81 0856

DOCUMENTS CONSIDERED TO BE RELEVANT			
Category	Citation of document with indication, where appropriate, of relevant passages	Relevant to claim	CLASSIFICATION OF THE APPLICATION (Int.Cl.7)
D,X	US 5 394 239 A (VALETTE SERGE) 28 February 1995 (1995-02-28)	1	G01N21/55
Y	* column 2, line 19-51 * * column 3, line 1-7 * * column 3, line 21-32; figures 1,2 *	2-6	
D,X	PANDRAUD G ET AL: "Evanescent wave sensing: new features for detection in small volumes" SENSORS AND ACTUATORS A, ELSEVIER SEQUOIA S.A., LAUSANNE, CH, vol. 85, no. 1-3, 25 August 2000 (2000-08-25), pages 158-162, XP004214464 ISSN: 0924-4247 * the whole document *	1	
Y	HUANG W ET AL: "ANALYSIS OF FOLDED ERBIUM-DOPED PLANAR WAVEGUIDE AMPLIFIERS BY THE METHOD OF LINES" JOURNAL OF LIGHTWAVE TECHNOLOGY, IEEE. NEW YORK, US, vol. 17, no. 12, 1 December 1999 (1999-12-01), pages 2658-2664, XP001006889 ISSN: 0733-8724 * page 2658, left-hand column, last paragraph; figure 1B *	2-6	
Y	US 5 701 372 A (BOYSEL ROBERT M ET AL) 23 December 1997 (1997-12-23) * column 4, line 18-26; figure 3 *	2-6	
Y	US 5 289 256 A (GRAMLING HUBERT) 22 February 1994 (1994-02-22) * column 9, line 21-53; figure 5 *	2-6	
-/--			
The present search report has been drawn up for all claims			
Place of search		Date of completion of the search	Examiner
MUNICH		9 January 2002	Meyer, F
CATEGORY OF CITED DOCUMENTS			
X : particularly relevant if taken alone Y : particularly relevant if combined with another document of the same category A : technological background O : non-written disclosure P : intermediate document		T : theory or principle underlying the invention E : earlier patent document, but published on, or after the filing date D : document cited in the application L : document cited for other reasons & : member of the same patent family, corresponding document	

EPO FORM 1503 03 82 (P04C01)

**CLAIMS INCURRING FEES**

The present European patent application comprised at the time of filing more than ten claims.

- Only part of the claims have been paid within the prescribed time limit. The present European search report has been drawn up for the first ten claims and for those claims for which claims fees have been paid, namely claim(s):
- No claims fees have been paid within the prescribed time limit. The present European search report has been drawn up for the first ten claims.

LACK OF UNITY OF INVENTION

The Search Division considers that the present European patent application does not comply with the requirements of unity of invention and relates to several inventions or groups of inventions, namely:

see sheet B

- All further search fees have been paid within the fixed time limit. The present European search report has been drawn up for all claims.
- As all searchable claims could be searched without effort justifying an additional fee, the Search Division did not invite payment of any additional fee.
- Only part of the further search fees have been paid within the fixed time limit. The present European search report has been drawn up for those parts of the European patent application which relate to the inventions in respect of which search fees have been paid, namely claims:
- None of the further search fees have been paid within the fixed time limit. The present European search report has been drawn up for those parts of the European patent application which relate to the invention first mentioned in the claims, namely claims:

1-6



European Patent
Office

EUROPEAN SEARCH REPORT

Application Number
EP 01 81 0856

DOCUMENTS CONSIDERED TO BE RELEVANT			
Category	Citation of document with indication, where appropriate, of relevant passages	Relevant to claim	CLASSIFICATION OF THE APPLICATION (Int.Cl.7)
Y	HOVEN VAN DEN G N ET AL: "NET OPTICAL GAIN AT 1.53 UM IN ER-DOPED AI2O3 WAVEGUIDES ON SILICON" APPLIED PHYSICS LETTERS, AMERICAN INSTITUTE OF PHYSICS. NEW YORK, US, vol. 68, no. 14, 1 April 1996 (1996-04-01), pages 1886-1888, XP000585100 ISSN: 0003-6951 * figure 1 *	2-6	
			TECHNICAL FIELDS SEARCHED (Int.Cl.7)
-The present search report has been drawn up for all claims-			
Place of search: MUNICH		Date of completion of the search: 9 January 2002	Examiner: Meyer, F
CATEGORY OF CITED DOCUMENTS X : particularly relevant if taken alone Y : particularly relevant if combined with another document of the same category A : technological background O : non-written disclosure P : intermediate document		T : theory or principle underlying the invention E : earlier patent document, but published on, or after the filing date D : document cited in the application L : document cited for other reasons & : member of the same patent family, corresponding document	

EPO FORM 1503 03/82 (P04/C01)



The Search Division considers that the present European patent application does not comply with the requirements of unity of invention and relates to several inventions or groups of inventions, namely:

1. Claims: 1-6

Claims 2 and 6: A sensor system for the detection of chemical substances (according to claim 1) in which the integrated optical waveguide has the form of (at least one) non-crossing spiral.

2. Claim : 7

Claim 7: A sensor system for the detection of chemical substances (according to claim 1) in which the light source is wavelength modulated and the detection circuitry is adapted for fundamental and/or harmonics detection.

3. Claims: 8,10

Claim 8: A sensor system where the input and output fibers are elongated in such a way that the interferometric noise generated by these fibers can be eliminated.

4. Claim : 9

Claim 9: A method for the detection of chemical substances (using e.g. a system according to claim 1), the method providing signal enhancement.

5. Claim : 11

Claim 11: A method for the detection of chemical substances (using e.g. a system according to claim 1), the method providing noise rejection.

6. Claim : 12

Claim 12: A sensor system for the detection of chemical substances (e.g. according to claim 1) adapted to sequentially scan several wavelengths.

7. Claim : 13

Claim 13: A sensor system for the detection of chemical substances (e.g. according to claim 1) comprising different non-crossing optical waveguides interlaced on the same substrate.



The Search Division considers that the present European patent application does not comply with the requirements of unity of invention and relates to several inventions or groups of inventions, namely:

8. Claim : 14

Claim 14: A sensor system for the detection of chemical substances (e.g. according to claim 1) comprising several light sources which can be used in a sequence or in parallel..

**ANNEX TO THE EUROPEAN SEARCH REPORT
ON EUROPEAN PATENT APPLICATION NO.**

EP 01 81 0856

This annex lists the patent family members relating to the patent documents cited in the above-mentioned European search report.
The members are as contained in the European Patent Office EDP file on
The European Patent Office is in no way liable for these particulars which are merely given for the purpose of information.

09-01-2002

Patent document cited in search report	Publication date	Patent family member(s)	Publication date
US 5394239 A	28-02-1995	FR 2694630 A1	11-02-1994
		DE 69315766 D1	29-01-1998
		DE 69315766 T2	18-06-1998
		EP 0584005 A1	23-02-1994
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		IT 1262345 B	19-06-1996
		JP 2081113 C	09-08-1996
		JP 6094425 A	05-04-1994
		JP 7097017 B	18-10-1995

专利名称(译)	传感器系统包括用于检测化学物质的集成光波导		
公开(公告)号	EP1291642A1	公开(公告)日	2003-03-12
申请号	EP2001810856	申请日	2001-09-05
[标]申请(专利权)人(译)	LINDE医疗传感器		
申请(专利权)人(译)	LINDE医疗传感器AG		
当前申请(专利权)人(译)	LINDE医疗传感器AG		
[标]发明人	SALZMANN DANIEL		
发明人	DEPEURSINGE, CHRISTIAN DR. SALZMANN, DANIEL		
IPC分类号	G01N21/27 A61B5/00 G01N21/39 G01N21/55		
CPC分类号	A61B5/4821 A61B5/1455 G01N21/552		
代理机构(译)	BRAUN, 安德烈		
外部链接	Espacenet		

摘要(译)

用于检测化学物质的传感器系统具有光波导(6)，其产生穿透到相邻介质(7)中的消逝场，用于将光耦合到波导(6)中的光源(2)，以及检测电路(9)用于接收来自波导(6)的光并产生反射所感测的化学物质的输出信号(11)。在优选实施例中，波导具有双线，非交叉螺旋的形式。它由进入或减小的螺旋段(12)和由一对相对的中央半圆形段(14)连续地约束的输出或增加的螺旋段(13)组成。

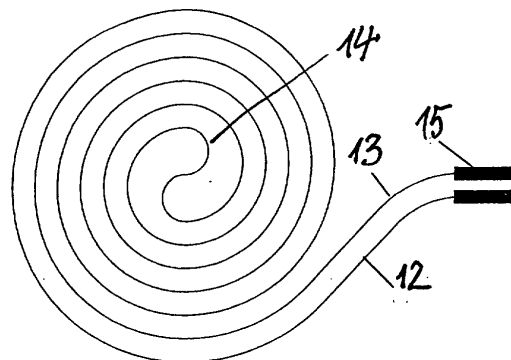


Fig. 3