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(54) Title: CAMERA FOR GENERATING A BIOMETRICAL SIGNAL OF A LIVING BEING

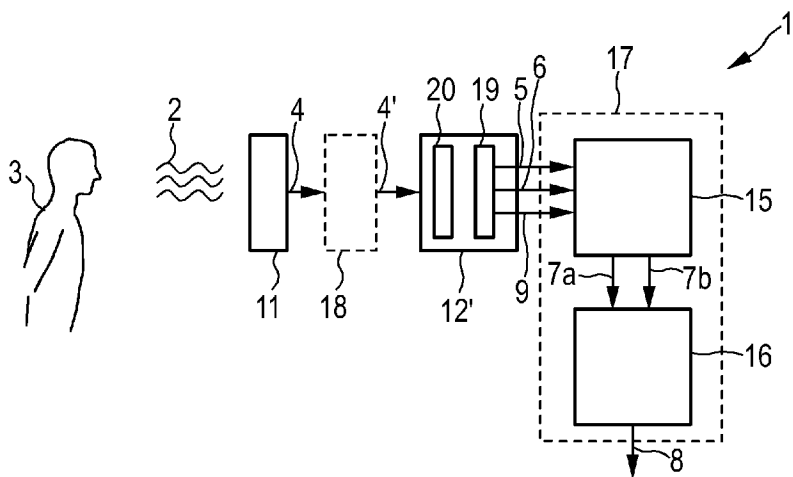


FIG. 2

(57) Abstract: The present invention relates to a camera (1, 1') for generating a biometrical signal of a living being comprising: a filter (11) for blocking incident visible light in a wavelength range up to at least 550 nm, a color sensor (12, 12') for receiving said filtered incident light and generating at least two different color signals (5, 6, 9), a combination unit (15) for generating at least one combined color signal (7a, 7b) by combining said at least two color signals, and a processing unit (16) for processing said at least one combined color signal and extracting at least one biometrical signal (8) of said living being (3).

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Camera for generating a biometrical signal of a living being

FIELD OF THE INVENTION

The present invention relates to a camera for generating a biometrical signal of a living being. The present invention relates further to a method for generating a biometrical signal of a living being. Still further, the present invention relates to a processor and a
5 processing method for use in such a camera and method. Finally, the present invention relates to a computer program for implementing said processing method.

BACKGROUND OF THE INVENTION

Pulse oximetry is a non-invasive method allowing a monitoring of the
10 oxygenation of a patient's hemoglobin using a pulse oximeter. A sensor is placed on a thin part of a patient's body, usually a finger tip or earlobe. Red light with a wavelength around 650 nm and infrared light with a wavelength around 850 to 940 nm are sequentially passed through the patient to a photodetector. The changing absorbance of each of the two
15 wavelengths is measured, allowing determination of the absorbances due to the pulsing arterial blood alone, excluding venous blood, skin, bone, muscle and fat. Based upon the ratio of changing absorbance of the red and infrared light caused by the difference in color between oxygen-bound (bright red) and oxygen-unbound (dark red or blue in severe cases) blood hemoglobin, a measure of oxygenation (the percent of hemoglobin molecules bound with oxygen molecules) can be made. This is also called SpO₂ monitoring in the art.

20 Camera-based SpO₂ monitoring is conventionally realized by two monochrome cameras with corresponding optical band-pass filters, but this is non-practical due to the required alignment (i.e. spatial alignment of the images from two or more sensors), complexity and costs for many applications, such as applications in sports, home-use or for implementation in smart devices, such as mobile phones.

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SUMMARY OF THE INVENTION

It is an object of the present invention to provide a camera and a corresponding method for generating a biometrical signal of a living being that can be applied in a wider range of applications and that are less complex and expensive compared to

conventional camera-based monitoring equipment and methods. It is a further object of the present invention to provide a corresponding processor and processing method for use in such a camera as well as a computer program for implementing said processing method.

In a first aspect of the present invention a camera is presented comprising:

- 5 - a filter for blocking incident visible light in a wavelength range up to at least 550 nm, in particular up to at least 600 nm,
- a color sensor for receiving said filtered incident light and generating three different color signals,
- a combination unit for generating at least one combined color signal by
- 10 combining said at least two color signals, and
- a processing unit for processing said at least one combined color signal and extracting at least one biometrical signal of said living being.

In a further aspect of the present invention a processor for use in a camera for generating a biometrical signal of a living being is presented comprising:

- 15 - a combination unit for generating at least one combined color signal by combining said at least two color signals, and
- a processing unit for processing said at least one combined color signal and extracting at least one biometrical signal of said living being.

In a further aspect of the present invention corresponding methods are

20 presented as well as a computer program comprising program code means for causing a computer to carry out the steps of the processing method when said computer program is carried out on the computer.

Preferred embodiments of the invention are defined in the dependent claims. It shall be understood that the claimed method has similar and/or identical preferred

25 embodiments as the claimed device and as defined in the dependent claims.

The present invention is based on the idea to add a special filter to a camera for generating a biometrical signal (also called vital sign) of a living being. While in conventional cameras a filter is used that blocks incident infrared light so that mainly visible light is sensed by a color sensor, e.g. an RGB sensor, according to the present invention quite

30 the contrary is proposed and a filter is used that blocks incident visible light in a wavelength range up to at least 550 nm, preferably up to at least 600 nm. In other words, the spectral characteristics of the camera are modified by placing a filter for blocking incident visible light in the optical path of the camera so that only light above a certain threshold wavelength hits the color sensor.

The color sensor generates at least two different color signals. These color signals are combined into at least one combined color signal which is then further processed to extract the desired biometrical signal. The result is an inexpensive and rather simple camera with near optimal spectral characteristics for biometrical signal detection, in particular for SpO₂ monitoring and SpO₂ imaging.

The invention is, however, not restricted to the detection of an SpO₂ signal, but may also extract other biometrical signals, such as heart beat, cardiac cycle, respiratory rate, depth of anesthesia or hypo- and hypervolemia of the living being. For instance, heart beat (also called heart rate or HR) detection from the at least one combined color signal is more robust with the proposed camera and method and can even be done under near dark illumination conditions since, according to the present invention, mainly the infrared light is evaluated rather than visible light as is conventionally done.

In a preferred embodiment the color sensor is adapted for generating three different color signals, preferably a red color signal, a green color signal and a blue color signal. Of course, these color sensors also have a sensitivity in the infrared wavelength range. The color sensor is preferably a standard RGB sensor including a photo detector and a color filter array for filtering the incident light differently before hitting the photo detector. In another embodiment the color sensor comprises a separate (different) color detectors for detecting different spectral parts of the incident light and generating different color signals.

In general, CCD/CMOS sensor manufacturers offer such sensors in monochrome (i.e. without color filters) and RGB (i.e. with a color filter array "printed" on top of the pixels) versions. The spectral response of those filters is optimized for the visible band. Increasing transparency of green and blue filters in near-infrared band (where the silicon of the sensor is still sensitive) is a side effect of the used chemicals (dyes). It is normally solved by equipping color cameras with IR-block filters by default.

The present invention can thus also be understood as a kind of misuse of such color sensors, in particular RGB color sensors (and their undesired behavior in the near infrared spectral range) trying to obtain a signal that would otherwise require different custom made optical filters.

The main reason for preferably using a standard, commercially available RGB sensor, is a cost factor (these sensors are made in huge volumes). Custom made color arrays are expensive when manufactured in low numbers. Using more than one monochrome sensor with optical filters, which is generally possible as well, but increases the total system cost as

well. Additionally, it introduces spatial alignment and/or perspective problems of the images from different sensors.

In another preferred embodiment the combination unit is adapted for combining said at least two color signals by a linear combination. Linear combinations have been shown to provide good results. But in certain circumstances, in particular dependent on
5 the kind of color sensor and/or the spectrum of the light source illuminating the living being, other combinations might be used alternatively.

In another embodiment the combination unit is adapted for generating two combined color signals by making two different combinations, in particular linear
10 combinations, of at least two of said three generated color signals. A good combination is a combination that minimizes cross-talk between said at least two combined color signals and thus maximizing contrast in the resulting biometrical signal. For instance, if the biometrical signal is extracted from the combined color signals by PPG (photoplethysmography) extraction the contrast between PPG amplitudes may thus be maximized.

A preferred combination leading to good results generates a first combined
15 color signal by adding the red color signal and the green color signal and subtracting two times the blue color signal from said sum and generates a second combined color signal by subtracting the green color signal from two times the blue color signal.

In another embodiment said filter is adapted for blocking incident visible light
20 in a wavelength range up to at least 650 nm. Generally, blue and green color detectors have a local minimum in light transmission in the wavelength range around 650 nm. It is preferred to block, however, a green sensitivity peak in the visible spectrum which is generally centered around 545 nm. A threshold at a longer wavelength above 650 nm is not preferred since this would reduce the contrast for the biometrical signal detection. Those biometrical
25 signals generally have minima in a wavelength range around 660 nm which thus represents a wavelength range in which the detection of the biometrical signal or the evaluation of a biometrical signal can best be done.

Naturally, in imaging silicon sensors, as preferably used in the color sensor, the sensitivity decreases towards longer wavelengths. If, however, this is not the case for a
30 certain color sensors another filter may be placed in the optical path of the camera that blocks incident light in a wavelength range above at least 1100 nm, in particular above at least 1000 nm, before reaching said color sensor.

As mentioned above, the proposed camera may be used for generating different kinds of biometrical signals. One field of a preferred application of the present

invention is for extracting a heart beat signal from that at least one combined color signal by PPG extraction.

A method to measure skin colour variations, called Photo-Plethysmographic imaging (PPG), is described in Wim Verkruysse, Lars O. Svaasand, and J. Stuart Nelson, "Remote plethysmographic imaging using ambient light", Optics Express, Vol. 16, No. 26, December 2008. It is based on the principle that temporal variations in blood volume in the skin lead to variations in light absorptions by the skin. Such variations can be registered by a video camera that takes images of a skin area, e.g. the face, while processing calculates the pixel average over a manually selected region (typically part of the cheek in this system). By looking at periodic variations of this average signal, the heart beat rate and respiratory rate can be extracted.

Thus, the pulsation of arterial blood causes changes in light absorption. Those changes observed with a photodetector (or an array of photodetectors) form a PPG (photo-plethysmography) signal (also called, among other, a pleth wave). Pulsation of the blood is caused by the beating heart, i.e. peaks in the PPG signal correspond to the individual beats of the heart. Therefore, a PPG signal is a heartbeat signal in itself. The normalized amplitude of this signal is different for different wavelengths, and for some wavelengths it is also a function of blood oxygenation.

To improve robustness of heart rate calculation, it is beneficial to use more than one PPG signal, in particular signals obtained at different wavelengths in such a way, that the difference of normalized amplitudes is maximized. Division of one signal by the other helps to eliminate distortions present in both signals.

Another field of application of the present invention is SpO₂ estimation. Thus, preferably, the processing means is adapted for extracting a SpO₂ signal from said at least one combined color signal by extracting at least two PPG signals at different wavelengths and determining a SpO₂ signal from said at least two PPG signals.

SpO₂ estimation is based on the ratio of the normalized amplitudes of PPG signal at two different ranges of wavelengths (one at red and the other at infra-red part of the spectrum):

$$RR = \frac{\frac{AC_{IR}}{DC_{IR}}}{\frac{AC_R}{DC_R}}$$

From this “ratio of ratios”, the SpO₂ value is obtained using experimentally defined constants C₁ and C₂

$$5 \quad SpO_2 = C_1 - \frac{C_2}{RR}.$$

The biometrical signal being directly measured is the PPG signal. SpO₂ is calculated from two PPG signals. Similarly, other mentioned signals/properties (respiration, depth of anesthesia, etc.) are also derivatives of the PPG signal.

10

BRIEF DESCRIPTION OF THE DRAWINGS

These and other aspects of the invention will be apparent from and elucidated with reference to the embodiment(s) described hereinafter. In the following drawings

15 Fig. 1 shows a schematic diagram of a camera according to the present invention,

Fig. 2 shows a schematic diagram of another embodiment of a camera according to the present invention,

Fig. 3 shows a top view of a Bayer color filter array,

20 Fig. 4 shows a diagram illustrating the spectral characteristics of a conventional color sensor,

Fig. 5 shows the used spectral parts of three different color signals according to the present invention,

Fig. 6 shows the spectral sensitivities of two combined color signals generated according to the present invention,

25 Fig. 7 shows a diagram illustrating the normalized amplitude over the PPG amplitude spectra for one person and different SpO₂ saturation values,

Fig. 8 shows diagrams for a sensitivity and normalized amplitude to illustrate SpO₂ signal evaluation,

30 Fig. 9 shows diagrams for sensitivity and normalized amplitude illustrating HR signal evaluation, and

Figs. 10A to 10C show diagrams of the sensitivity of another sensor without and with a filter for blocking visible light and of two combined color channels.

DETAILED DESCRIPTION OF THE INVENTION

Fig. 1 shows a schematic diagram of a first embodiment of a camera 1 according to the present invention. Electromagnetic radiation 2, in particular light in the visible and infrared wavelength range, reflected from a living being 3, such as a patient, is received and evaluated by said camera 1 for finally generating the biometrical signal of the living being 3. The camera comprises a filter 11 for blocking incident visible light within the incident electromagnetic radiation 2 in a wavelength range up to at least substantially 550 nm, preferably up to approximately 600 nm, even more preferably up to 650 nm. The filtered incident light 4 is then sensed by a color sensor 12 that generates at least two different color signals 5, 6, e.g. by use of two separate color detectors 13, 14 (or an array of such color detectors). A combination unit 15 generates at least one combined color signal 7 by combining said color signals 5, 6, e.g. by a linear combination. Finally, a processing unit 16 is provided for processing said combined color signal 7 and extracting at least one biometrical signal 8 of the living being 3.

The combination unit 15 and the processing unit 16 are preferably realized at a common processor 17, e.g. are realized as processing elements of a processor or are implemented in software on a conventional processor. However, they may also be realized in a different manner, e.g. as dedicated hardware elements.

Fig. 2 schematically shows a second embodiment of a camera 1' according to the present invention. Fig. 2 shows that optionally an additional filter 18 may be provided (in this and/or other embodiments), which filter 18 is configured to block incident light in a wavelength range above at least 1100 nm, in particular above at least 1000 nm, before reaching the color sensor 12'. While generally those color sensors, e.g. imaging silicon sensors, show a sensitivity that naturally decreases towards longer wavelengths, such an additional filter 18 ensures that signal contributions within the filtered incident light 4 above said upper threshold wavelength are blocked, i.e. signal contributions in which water absorption becomes dominant are blocked in the twice filtered incident light 4'.

Further, in this embodiment the color sensor 12' generates three different color signals 5, 6, 9, e.g. by use of a color filter array 20 having three different color filter areas provided in front of a photo detector 19 (or, more generally, the image sensor). Such a color sensor (e.g. including a color filter array having only two color filter areas could also be used in the embodiment shown in Fig. 1. Preferably, the color sensor 12' comprises a color filter array generating a red color signal 5, a green color signal 6 and a blue color signal 9 as conventionally provided by an RGB color sensor.

From the three color signals 5, 6, 9 the combination unit 15 generates two combined color signals 7a, 7b by making two different combinations, in particular linear combinations, of at least two of said three color signals 5, 6, 9. From these two combined color signals 7a, 7b the processing unit then finally extracts the desired biometrical signal 8.

5 As explained above standard RGB cameras use a color filter array overlaid over pixels of the image sensor in a repetitive pattern. Such a Bayer color filter array 20 that can also be used according to the present invention is depicted in Fig. 3. Such a color filter array comprises a number of red filter areas 21, blue filter areas 22 and green filter areas 23. The spectral response is generally optimized for the visual representation of recorded images.
10 However, such standard RGB cameras are far from optimal for camera-based generation of biometrical signals of a living being, in particular for camera-based PPG extraction including the extraction of heart rate signals and SpO2 signals. An option would be the use of custom-made color filter arrays, but these are generally an expensive alternative.

Further, conventionally an IR filter blocking infrared light is placed in front of
15 the RGB camera to block infrared light.

According to the present invention, instead, the visible light is blocked with the filter 11 up to a predetermined threshold wavelength, typically in the range from 550 to 650 nm (e.g. around 600 nm), and no extra infrared filter is generally used. A color sensor 12 is preferably a conventional color sensor, such as a standard RGB sensor as used in an RGB
20 camera which, in an embodiment, may also include such a Bayer color filter array 20 as shown in Fig. 3 or any other means for providing at least two (preferably three) color signals.

The effects of the present invention shall be illustrated by way of an example assuming the use of a conventional RGB camera sensor including a Bayer color filter array. The spectral characteristics of such a Bayer color filter array are depicted in Fig. 4 showing
25 the sensitivity curve B for blue light, the sensitivity curve G for green light and the sensitivity curve R for red light. By default, conventional cameras are equipped with infrared block filters, as mentioned above, to block infrared light, particularly in the wavelength range above 650 nm, to avoid influence of light from outside the visible range. According to the present invention, however, such an IR block filter is removed and actually the visible part of
30 the sensitivity spectrum is blocked up to a threshold wavelength in the range from 550 to 650 nm as depicted in the diagram shown in Fig. 5 showing only the part of the spectra that are passing through the filter unit 11.

Next, in the combination unit 15, from these three color signals R, G, B (representing the color signals 5, 6, 9 in this example) to combined color signals 7a, 7b are

generated by linear combinations of the color signals. In particular, in an embodiment the first combined color signal Ch1 (e.g. representing combined color signal 7a) is defined as $Ch1 = R - 2b + G$ and the second combined color signal Ch2 (representing the second combined color signal 7b) is defined as $Ch2 = 2B - G$. The spectral sensitivities of combined color signals Ch1 and Ch2 are depicted in the diagram shown in Fig. 6. To be precise, this diagram does not show any signals, but a spectral sensitivity characteristic, where a signal is understood as a time varying value obtained by integration of light by those sensitivity curves.

Referring to the diagram shown in Fig. 4 showing an effective spectral characteristic of the color filter array and silicon sensitivity, which is generally the same for all pixels, it can be seen that going from a wavelength of 650 nm towards longer wavelengths, the filter areas of the color sensor more or less maintain their transmission level, while the blue and green filter areas of the color sensor are becoming more and more "transparent". At some wavelength around 830 nm the silicon sensitivity starts dropping down, which equally limits the light collection by all three color channels. Further, it can be seen that at a wavelength around 650 nm the blue and green filter areas have a local minimum in light transmission.

According to the present invention, it has been shown that it is desired to block the green filter peak in the visible spectrum which is around 545 nm. On the other hand, to avoid a severe reduction of the contrast the upper threshold wavelength of the filter unit should not be substantially higher than 700 nm, particularly not higher than 650 nm. The reason can be seen from the diagram shown in Fig. 7 showing PPG amplitude spectra for one person and different SpO₂ saturation values from 85% to 100%. Since it is desired to capture the minima of these curves, which minima are around 660 nm, the upper threshold wavelength of the filter unit should not be above the wavelength of these minima.

The present invention thus provides the option to build a very inexpensive camera for generating a biometrical signal of a living being, in particular of an SpO₂ signal and/or heart rate signal. Fig. 8A show the sensitivity for the two combined color signals Ch1 and Ch2 as explained above, and Fig. 8B shows the PPG amplitude spectra as depicted in Fig. 7. As indicated by the vertical line through 800 nm the two combined color signals Ch1 and Ch2 are now near optimal SpO₂ wavelength bands, similar to those as obtained in conventional pulse oximetry. As mentioned above, conventional pulse oximetry uses a red band (around 660 nm), where a significant difference in light absorption between oxy- and deoxyhemoglobin exists, and an infra-red band (850-940 nm), where this difference is much

smaller and in the opposite direction. A wavelength of 800 nm is an isosbestic point of the hemoglobin, i.e. both oxy- and deoxyhemoglobin have the same light absorption.

As explained above a SpO₂ signal is extracted from said at least one combined color signal by extracting at least two PPG signals at different wavelengths and determining a SpO₂ signal from said at least two PPG signals.

Fig. 9A also shows the two combined color signals Ch1, Ch2 as explained above, and Fig. 9B shows unstable PPG amplitudes due to variations between individuals in the visible wavelength range as indicated by arrow 30. The variations in the amplitude are for different individuals (different modeled skin physiologies) and not due to the oxygenations levels. As shown in these diagrams, for a simple detection of the heart rate a good stable contrast in amplitude between the two channels Ch1, Ch2 is desired as is given in this case. The conventionally used green wavelength range (500 to 600 nm) is strong in amplitude, but not stable. As explained above a conventional PPG extraction algorithm can be applied to the two channels to obtain a PPG signal representing the heartbeat signal.

Figs. 10A to 10C show corresponding diagrams for a different color sensor. Fig. 10A shows a diagram of the spectral characteristic of the color sensor and Fig. 10B shows a diagram of the spectral characteristic of said color sensor with a filter blocking visible light. Fig. 10C shows a diagram of the virtual color channels Ch1 and Ch2 resulting from a combination of RGB, where $Ch1 = R - B$ and $Ch2 = 1.5 * B - 0.5 * G$.

While the invention has been illustrated and described in detail in the drawings and foregoing description, such illustration and description are to be considered illustrative or exemplary and not restrictive; the invention is not limited to the disclosed embodiments. Other variations to the disclosed embodiments can be understood and effected by those skilled in the art in practicing the claimed invention, from a study of the drawings, the disclosure, and the appended claims.

In the claims, the word "comprising" does not exclude other elements or steps, and the indefinite article "a" or "an" does not exclude a plurality. A single element or other unit may fulfill the functions of several items recited in the claims. The mere fact that certain measures are recited in mutually different dependent claims does not indicate that a combination of these measures cannot be used to advantage.

A computer program may be stored/distributed on a suitable non-transitory medium, such as an optical storage medium or a solid-state medium supplied together with or as part of other hardware, but may also be distributed in other forms, such as via the Internet or other wired or wireless telecommunication systems.

Any reference signs in the claims should not be construed as limiting the scope.

CLAIMS:

1. Camera for generating a biometrical signal of a living being comprising:
 - a filter (11) for blocking incident visible light in a wavelength range up to at least 550 nm,
 - a color sensor (12, 12') for receiving said filtered incident light and generating at least two different color signals,
 - a combination unit (15) for generating at least one combined color signal by combining said at least two color signals, and
 - a processing unit (16) for processing said at least one combined color signal and extracting at least one biometrical signal of said living being.
2. Camera as claimed in claim 1, wherein said color sensor (12) is adapted for generating at least three color signals.
3. Camera as claimed in claim 2, wherein said color sensor (12') is adapted for generating a red color signal, a green color signal and a blue color signal.
4. Camera as claimed in claim 1, wherein said combination unit (15) is adapted for combining said at least two color signals by a linear combination.
5. Camera as claimed in claim 2, wherein said combination unit (15) is adapted for generating two combined color signals by making two different combinations, in particular linear combinations, of at least two of said three color signals.
6. Camera as claimed in claim 3, wherein said combination unit (15) is adapted for generating a first combined color signal by adding the red color signal and the green color signal and subtracting two times the blue color

signal from said sum and for generating a second combined color signal by subtracting the green color signal from two times the blue color signal.

7. Camera as claimed in claim 1,

5 wherein said filter (11) is adapted for blocking incident visible light in a wavelength range up to at least 650 nm.

8. Camera as claimed in claim 1,

10 further comprising another filter (18) for blocking incident light in a wavelength range above at least 1100 nm, in particular above at least 1000 nm, before reaching said color sensor.

9. Camera as claimed in claim 1,

15 wherein said processing unit (16) is adapted for extracting a heartbeat, cardiac cycle, respiratory rate, SpO₂, depth of anesthesia or hypo- and hypervolemia of the living being from said at least one combined color signal.

10. Camera as claimed in claim 1,

20 wherein said processing unit (16) is adapted for extracting a SpO₂ signal from said at least one combined color signal by extracting at least two PPG signals at different wavelengths and determining a SpO₂ signal from said at least two PPG signals.

11. Camera as claimed in claim 1,

25 wherein said processing unit (16) is adapted for extracting a heartbeat signal from said at least one combined color signal by PPG extraction

12. Method for generating a biometrical signal of a living being comprising the steps of:

- blocking incident visible light in a wavelength range up to at least 550 nm,
- receiving said filtered incident light by a color sensor,
- 30 - generating at least three different color signals,
- generating at least one combined color signal by combining said at least two color signals, and
- processing said at least one combined color signal and extracting at least one biometrical signal of said living being.

13. Processor for use in a camera for generating a biometrical signal of a living being, said camera comprising a filter for blocking incident visible light in a wavelength range up to at least 550 nm and a color sensor for receiving said filtered incident light and generating at least two different color signals, said processor (17) comprising:

- a combination unit (15) for generating at least one combined color signal by combining said at least two color signals, and
- a processing unit (16) for processing said at least one combined color signal and extracting at least one biometrical signal of said living being.

14. Processing method for use in a camera for generating a biometrical signal of a living being, said camera comprising a filter for blocking incident visible light in a wavelength range up to at least 550 nm and a color sensor for receiving said filtered incident light and generating at least two different color signals, said processing method comprising:

- generating at least one combined color signal by combining said at least two color signals, and
- processing said at least one combined color signal and extracting at least one biometrical signal of said living being.

15. Computer program comprising program code means for causing a computer to carry out the steps of the method as claimed in claim 14 when said computer program is carried out on the computer.

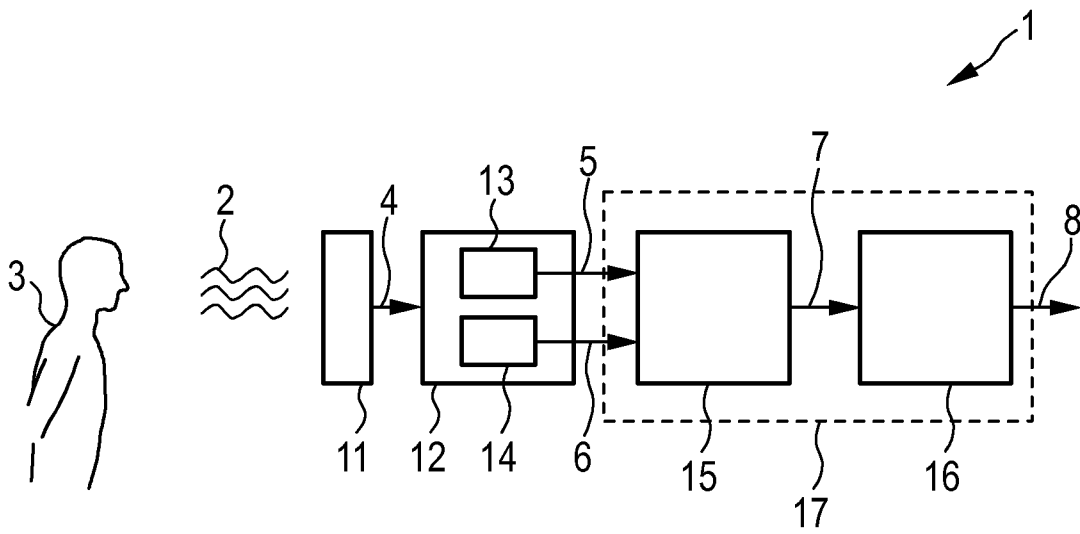


FIG. 1

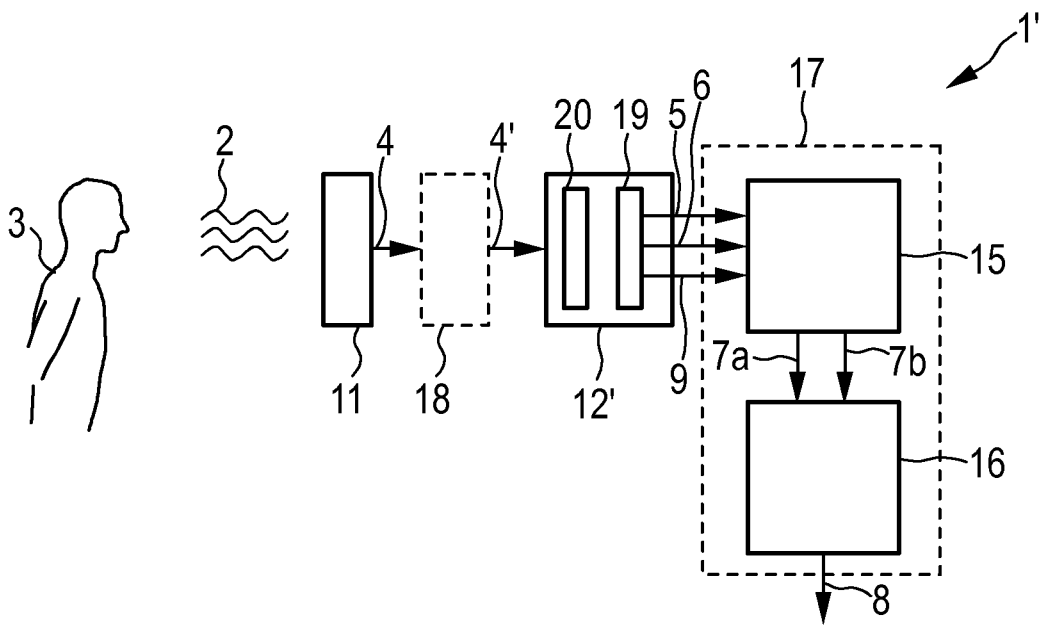


FIG. 2

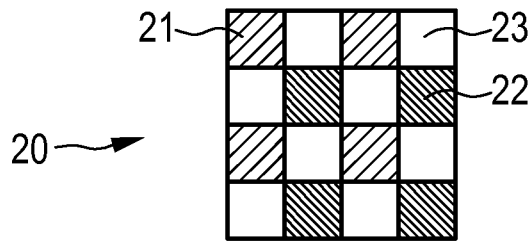


FIG. 3

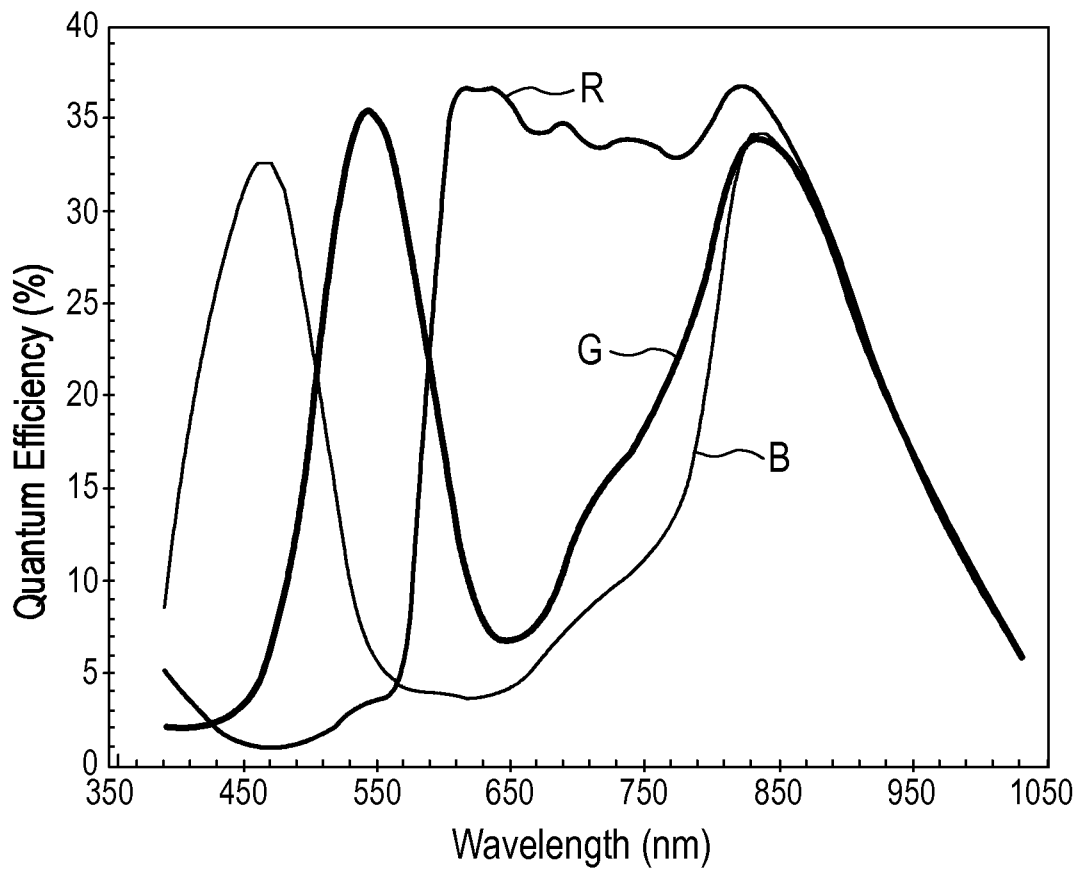


FIG. 4

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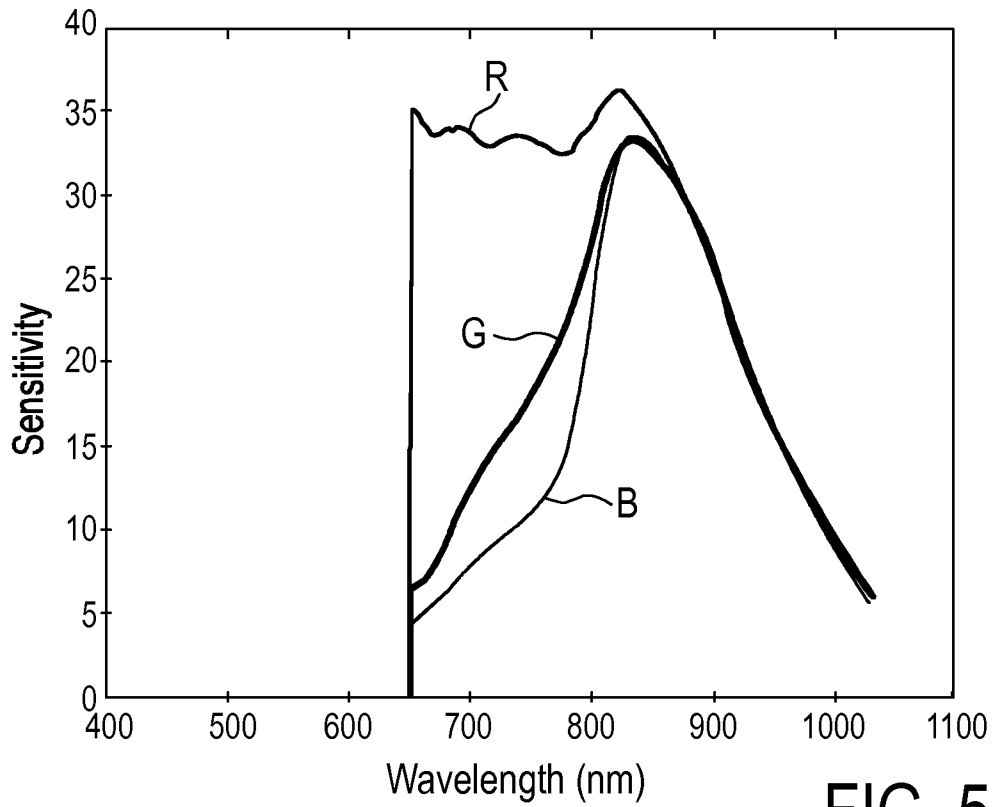


FIG. 5

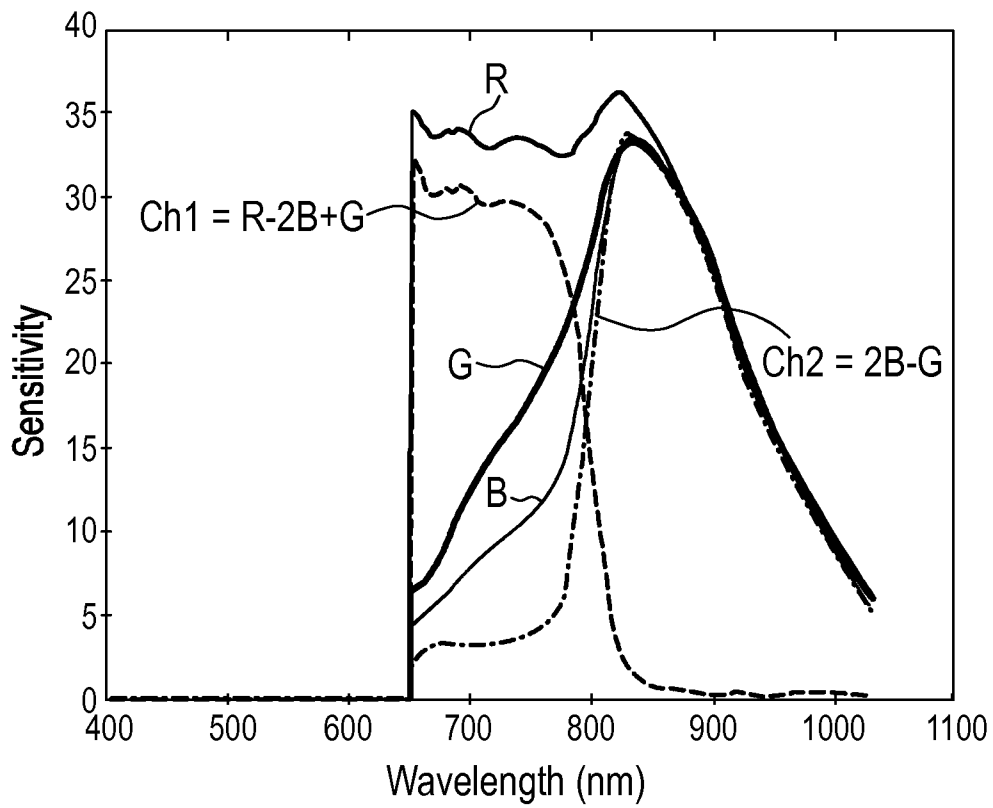


FIG. 6

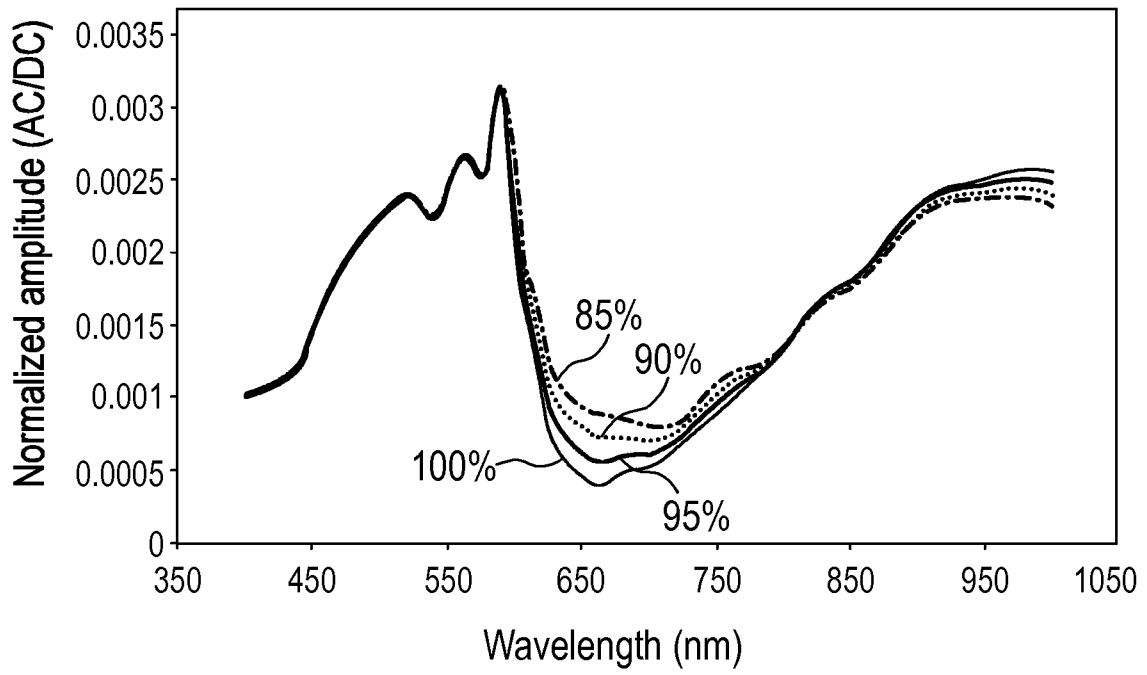


FIG. 7

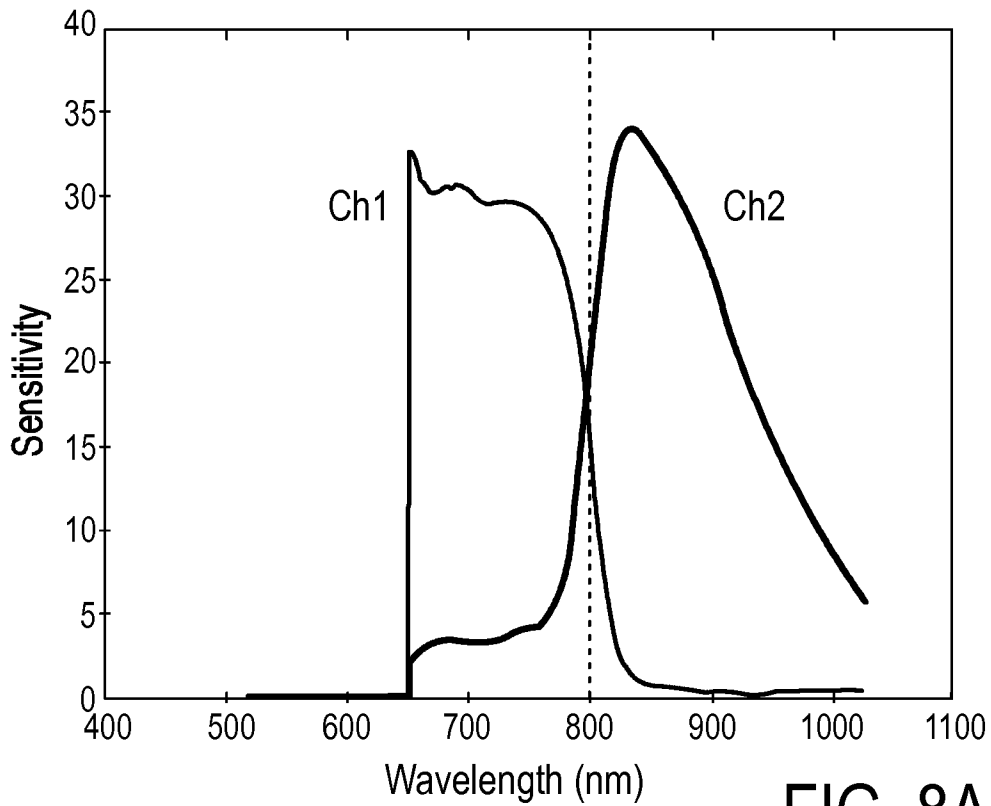


FIG. 8A

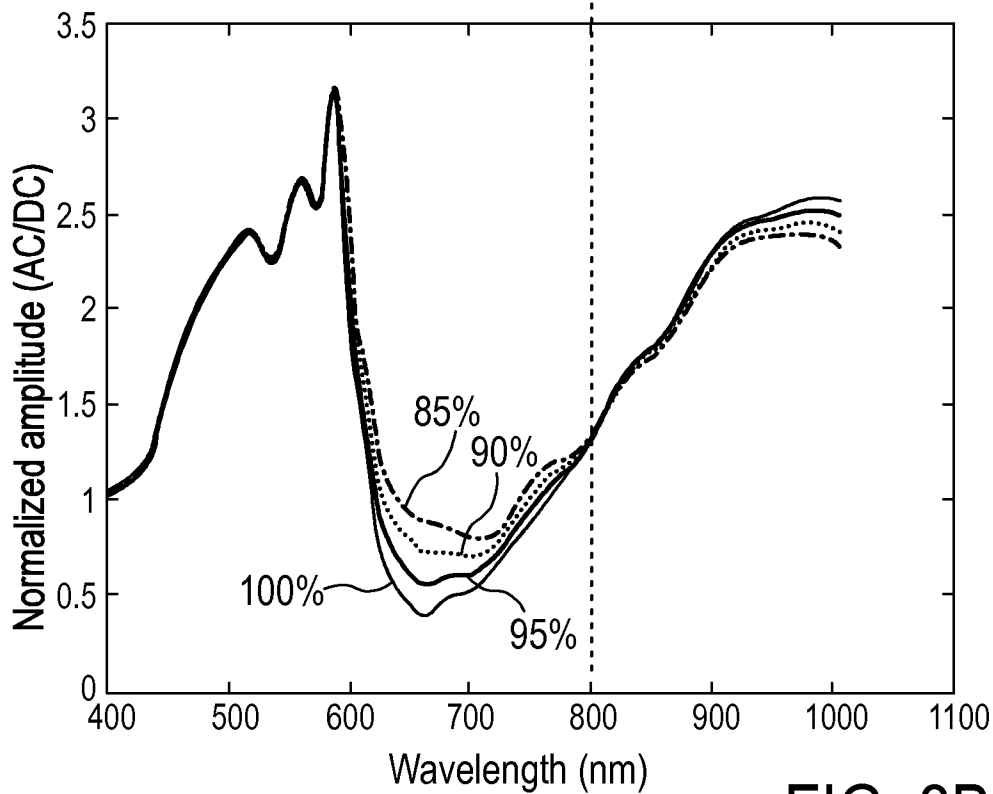


FIG. 8B

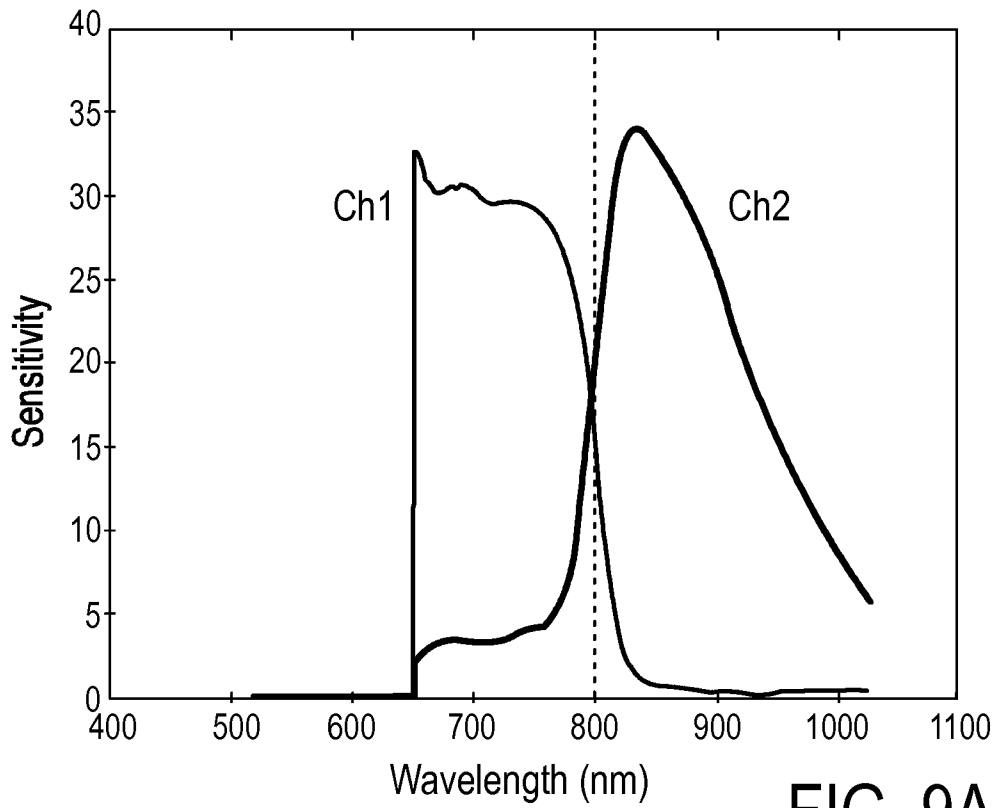


FIG. 9A

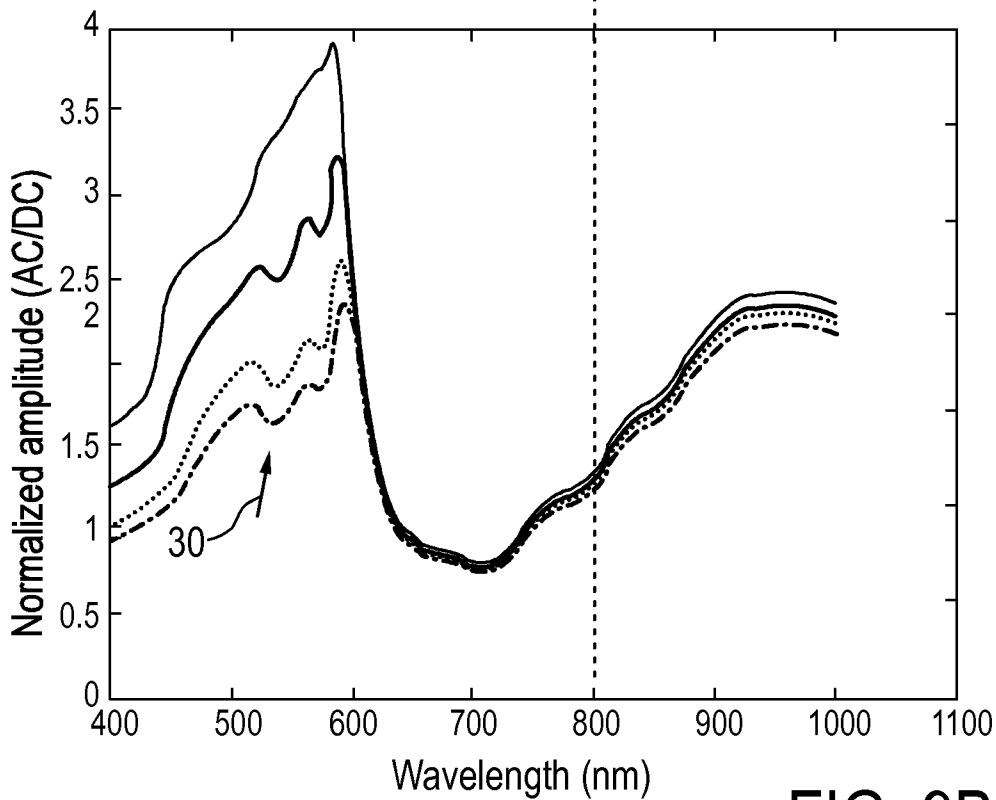


FIG. 9B

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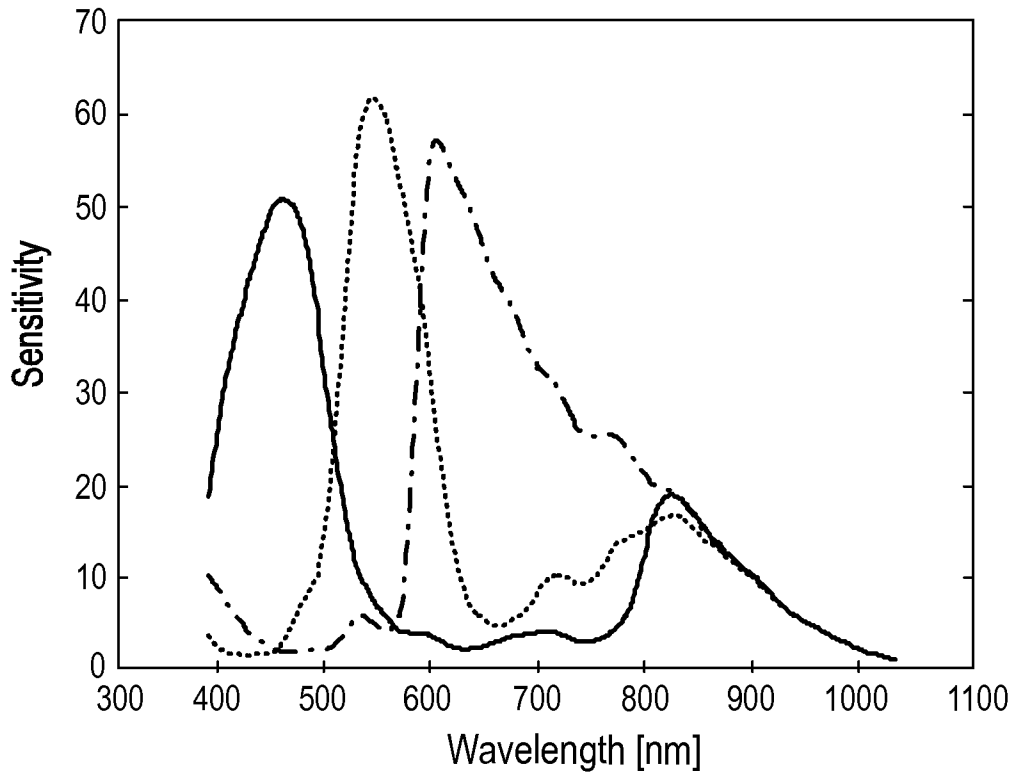


FIG. 10A

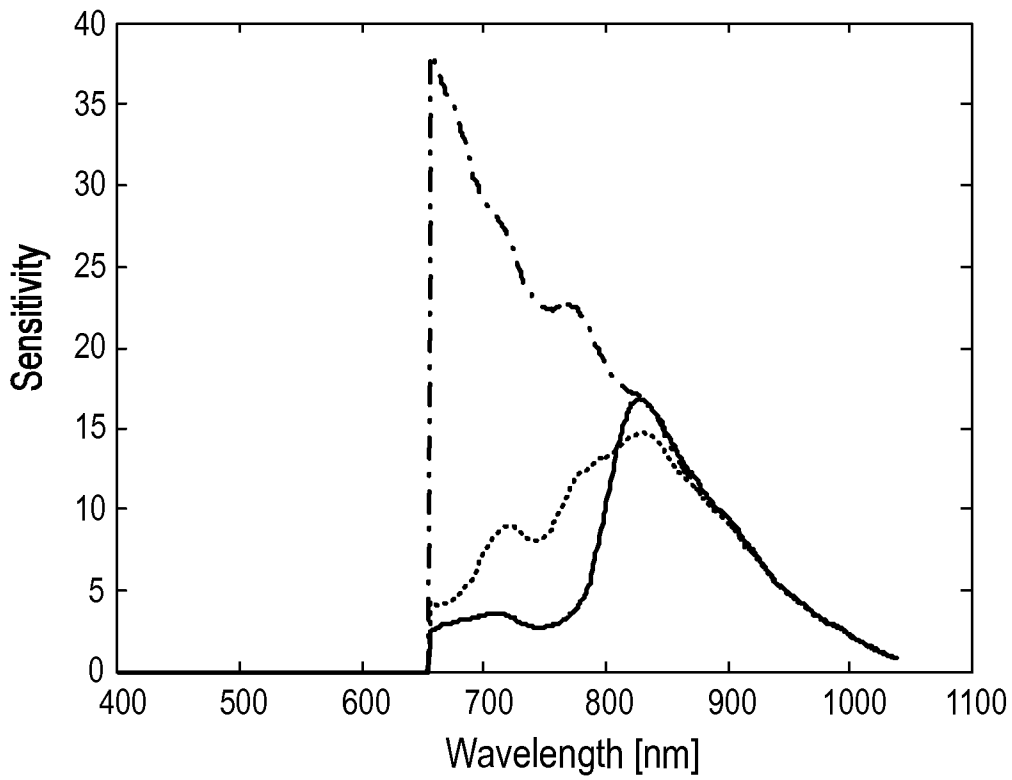


FIG. 10B

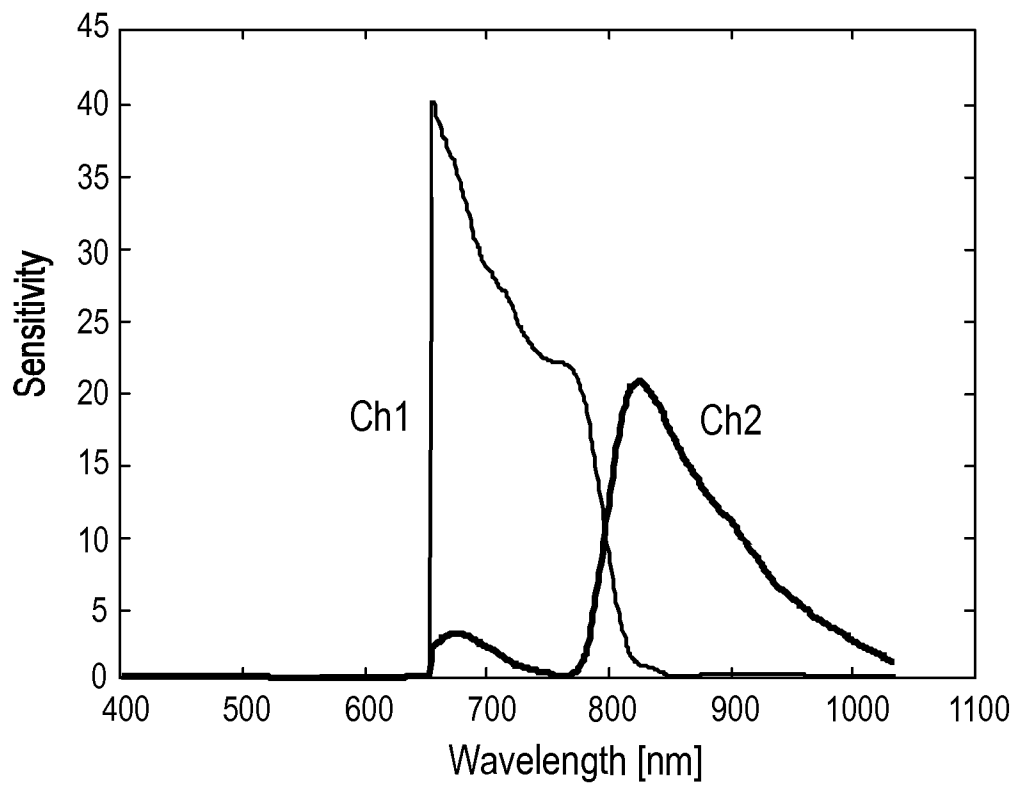


FIG. 10C

INTERNATIONAL SEARCH REPORT

International application No
PCT/IB2012/054375

A. CLASSIFICATION OF SUBJECT MATTER
 INV. A61B5/024 A61B5/1455 A61B5/00 G06T7/00
 ADD. G06K9/00

According to International Patent Classification (IPC) or to both national classification and IPC

B. FIELDS SEARCHED

Minimum documentation searched (classification system followed by classification symbols)
 A61B G06T

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

Electronic data base consulted during the international search (name of data base and, where practicable, search terms used)

EPO-Internal

C. DOCUMENTS CONSIDERED TO BE RELEVANT

Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X	WO 2011/042839 A1 (KONINKL PHILIPS ELECTRONICS NV [NL]; KIRENKO IHOR OLEHOVYCH [NL]; JEAN) 14 April 2011 (2011-04-14) the whole document	1-15
A	US 2008/306372 A1 (OHKI MITSU HARU [JP] ET AL) 11 December 2008 (2008-12-11) paragraphs [0025], [0026]	1-15
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 Further documents are listed in the continuation of Box C. See patent family annex.

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Date of the actual completion of the international search

4 January 2013

Date of mailing of the international search report

16/01/2013

Name and mailing address of the ISA/

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Authorized officer

Schindler, Martin

INTERNATIONAL SEARCH REPORT

International application No
PCT/IB2012/054375

C(Continuation). DOCUMENTS CONSIDERED TO BE RELEVANT		
Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
A	MADHU MOHAN N ET AL: "Contact-less, Multi-Spectral Imaging of Dermal Perfusion", INSTRUMENTATION AND MEASUREMENT TECHNOLOGY CONFERENCE PROCEEDINGS, 2008. IMTC 2008. IEEE, IEEE, PISCATAWAY, NJ, USA, 12 May 2008 (2008-05-12), pages 793-796, XP031274705, ISBN: 978-1-4244-1540-3 the whole document -----	1-15
A	US 2003/163032 A1 (TERRY ALVIN MARK [US]) 28 August 2003 (2003-08-28) paragraphs [0052] - [0060]; figure 4 -----	1-15

INTERNATIONAL SEARCH REPORT

Information on patent family members

International application No

PCT/IB2012/054375

Patent document cited in search report	Publication date	Patent family member(s)	Publication date
WO 2011042839 A1	14-04-2011	CN 102576458 A	11-07-2012
		EP 2486539 A1	15-08-2012
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		WO 03071941 A1	04-09-2003

专利名称(译)	用于生成生物的生物信号的相机		
公开(公告)号	EP2741661A1	公开(公告)日	2014-06-18
申请号	EP2012772473	申请日	2012-08-27
[标]申请(专利权)人(译)	皇家飞利浦电子股份有限公司		
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发明人	BARTULA, MAREK, JANUSZ VERKRUIJSSE, WILLEM		
IPC分类号	A61B5/024 A61B5/1455 A61B5/00 G06T7/00 G06K9/00		
CPC分类号	A61B5/02427 A61B5/14551 G06T7/0016 G06T2207/10024 G06T2207/30076 G06T7/0012		
代理机构(译)	STEFFEN , THOMAS		
优先权	61/530546 2011-09-02 US		
其他公开文献	EP2741661B1		
外部链接	Espacenet		

摘要(译)

本发明涉及一种用于产生生物的生物统计信号的照相机 (1,1') , 包括 : 用于阻挡波长范围高达至少550nm的入射可见光的滤光器 (11) , 颜色传感器 (12) 12') 用于接收所述滤波的入射光并产生至少两个不同的颜色信号 (5,6,9) , 组合单元 (15) 用于通过至少组合所述至少一个组合的颜色信号 (7a , 7b) 两个颜色信号 , 和处理单元 (16) , 用于处理所述至少一个组合颜色信号并提取所述生物 (3) 的至少一个生物统计信号 (8) 。