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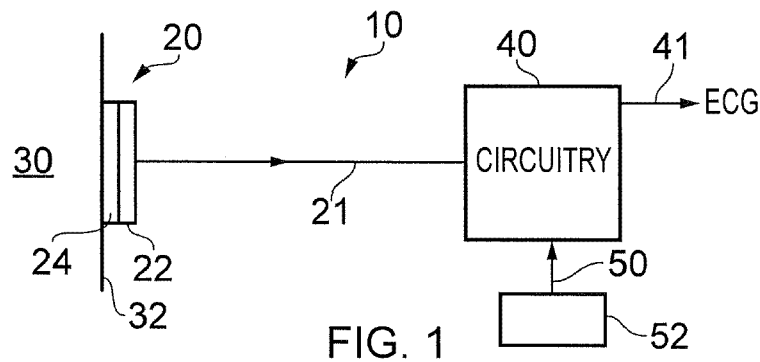
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(54) **BIO-SIGNAL DETECTION**

(57) an apparatus comprising:
 a displacement current sensor configured to measure a sensed signal dependent upon electrical activity of a sub-

ject's heart; and
 circuitry configured to process the sensed signal to compensate for artefacts arising from motion of the subject.



Description

TECHNOLOGICAL FIELD

[0001] Embodiments of the present invention relate to bio-signal detection. In particular, they relate to improving bio-signal detection.

BACKGROUND

[0002] Bio-signals are signals that provide information about the functioning of a subject's body. There are a very large number of bio-signals.

[0003] Bio-signals that relate to the heart and circulation include, for example, systolic blood pressure, diastolic blood pressure, heart rate, electrocardiogram, pulse wave velocity, phonocardiogram, ballistocardiogram, echocardiogram etc.

[0004] Detected bio-signals can suffer from noise arising from many different sources.

[0005] It is desirable to remove noise from bio-signals.

BRIEF SUMMARY

[0006] According to various, but not necessarily all, embodiments of the invention there is provided an apparatus comprising: a displacement current sensor configured to measure a sensed signal dependent upon electrical activity of a subject's heart; and circuitry configured to process the sensed signal to compensate for artefacts arising from motion of the subject.

[0007] According to various, but not necessarily all, embodiments of the invention there is provided examples as claimed in the appended claims.

BRIEF DESCRIPTION

[0008] For a better understanding of various examples that are useful for understanding the detailed description, reference will now be made by way of example only to the accompanying drawings in which:

Fig 1 illustrates an example of an apparatus for processing one or more sensed electrical signals to compensate for artefacts arising from motion of the subject.;

Figs 2 and 3 illustrates examples of an apparatus for processing one or more sensed electrical signals to compensate for artefacts arising from motion of the subject;

Fig 4 illustrates an example of a configuration of a guard electrode and an ECG electrode;

Fig 5 illustrates an example of a demodulation circuit; Figures 6A, 6B, 6C illustrate examples of motion-associated sensors which may, optionally, be fixed to articles;

Figs 7A to 7D illustrate further examples of circuitry configured to process the one or more sensed elec-

trical signals to compensate for artefacts arising from motion of the subject;

Fig 8 illustrates an example of a controller configured to process the one or more sensed electrical signals to compensate for artefacts arising from motion of the subject; and

Fig 9 illustrates an example of a method.

DETAILED DESCRIPTION

[0009] Fig 1 illustrates an example of an apparatus 10 for processing one or more sensed electrical signals 21 dependent upon electrical activity of a subject's heart; to compensate for artefacts arising from motion of the subject. In this way, in some examples, the apparatus 10 obtains an electrocardiogram signal 41 from the one or more sensed electrical signals 21. An electrocardiogram signal 41 is a signal that depends upon the electrical polarization and depolarization of the heart muscles. It is indicative of heart function.

[0010] The apparatus 10 may therefore be, or be a part of, a circulation monitoring system or a health monitoring system that uses the electrocardiogram signal 41 to assess heart function. This may find application for patient monitoring, for personal health monitoring, for fitness assessment, for exercise effectiveness monitoring etc.

[0011] The apparatus 10 comprises at least a displacement current sensor 20 and circuitry 40 operatively connected to the displacement current sensor 20. The connection may, for example, be a direct galvanic connection via a lead, as illustrated in Figs 2 and 3.

[0012] The displacement current sensor 20 is configured to measure one or more sensed electrical signals 21 dependent upon electrical activity of a heart of a subject 30. The sensor 20 detects the one or more sensed electrical signals 21. The sensor 20 may or may not further process the detected electrical signal to produce the one or more sensed electrical signals 21. Measurement does not therefore imply that the one or more sensed electrical signals is quantised, although it may be.

[0013] The total current density (defined by curl \mathbf{H}) has a galvanic component \mathbf{J} and a displacement component $d\mathbf{D}/dt$, where $\mathbf{D} = \epsilon\mathbf{E}$. The displacement current sensor 20 measures a value dependent upon \mathbf{D} and its variation over time, $d\mathbf{D}/dt$.

[0014] The displacement current sensor 20 comprises at least one electrode 22 in proximity to the skin 32 of the subject 30 but electrically insulated therefrom.

[0015] In some examples the displacement current sensor 20 comprises electrical insulation 24 for insulating the at least one electrode 22 from the subject's skin 32.

[0016] In some examples, material between the electrode 22 and the subject's skin 30 additionally or alternatively provides electrical insulation of the electrode 22 from the subject's skin 32.

[0017] The electrical insulation prevents the displacement current sensor 20 from receiving the galvanic component \mathbf{J} of the total current density.

[0018] The circuitry 40 is configured to process the one or more sensed electrical signals 21 to compensate for artefacts arising from motion of the subject. The compensation for motion artefacts removes noise from the sensed electrical signal 21 producing an electrical signal 21 less affected by noise.

[0019] The circuitry 40 receives a motion associated signal 50 that is associated with motion of the electrode 22 of the displacement current sensor 20 relative to the user 30.

[0020] For example, the motion associated signal 50 may be a motion dependent signal that is dependent upon or responsive to motion of the electrode 22 of the displacement current sensor 20 relative to the user 30. Additionally or alternatively, the motion associated signal 50 may be a force dependent signal that is dependent upon or responsive to force that causes motion of the electrode 22 of the displacement current sensor 20 relative to the user 30.

[0021] In some examples, the apparatus 10 comprises one or more motion-associated sensors 52 for producing one or more motion-associated signals 50.

[0022] For example, a motion-associated sensor 52 may be a motion sensor, a distance sensor; a force sensor, a pressure sensor, a deformation sensor and/or a body wearable motion sensor.

[0023] The motion-associated sensor 52 may, for example, be a capacitive sensor, a radio frequency sensor, an ultrasound sensor, an optical sensor; and electromagnetic film sensor, a piezoelectric sensor, a strain gauge sensor, an accelerometer, a gyroscope, and/or a magnetometer.

[0024] The circuitry 40 may be any suitable circuitry. It may be an arrangement of discrete components, and/or may comprise programmable gate arrays, and/or may comprise programmed processors, for example.

[0025] In some but not necessarily all examples, the circuitry 40 is configured to measure a variable capacitance caused by motion of the electrode 22 of the displacement current sensor 20 relative to the user 30. The circuitry 40 may be configured to measure a variable reactance caused by motion of the electrode 22 of the displacement current sensor 20 relative to the user 30 by measuring, in the Imaginary domain, modulation of a reference signal by the variable reactance. In the examples illustrated in Figs 2 and 3, the reference signal is an external signal 45 applied to the subject 30.

[0026] In the examples of Figs 2 and 3, the circuitry 40 is configured to process the one or more sensed electrical signals 21 to obtain a noise-reduced electrocardiogram signal 41. The circuitry 40 measures the artefacts caused by motion as a modulation of the electrical reference signal 45 provided to the subject 30 via the first electrode 26 by the circuitry 40. The circuitry 40 is configured to process the sensed signal 21 to compensate for the artefacts arising from motion of the subject.

[0027] The circuitry 40 is configured to apply a time variable voltage V_1 , as the reference signal 45, to a first

electrode 26, for example via a first operational amplifier, and measure a time variable signal V_{out} , for example at an output of a second operational amplifier.

[0028] In these examples, the first electrode 26 is in proximity to the skin 32 of the subject 30 but electrically insulated therefrom. In some examples, electrical insulation 24 insulates the electrode 26 from the subject's skin 32. In some examples material between the electrode 26 and the subject's skin 30 additionally or alternatively provides electrical insulation of the electrode 26 from the subject's skin 32.

[0029] The electrical reference signal 45 has one or more high frequency components, for example, greater than 1 kHz. For example, the electrical reference signal 45 may have a significant component over 100kHz, for example in the range 100-500 kHz, or in some embodiments may lie entirely within the range over 100kHz or 100-500 kHz. The electrical reference signal 45 may, for example, be a pure tone (single frequency).

[0030] In the example of Fig 3, a first displacement current sensor 20₁ comprises a first ECG electrode 60₁ for measuring a first ECG signal 41₁, and a first electrode 26 for injection of a current (reference signal 45), and a second displacement current sensor 20₂ comprises a second ECG electrode 60₂ for measuring a second ECG signal 41₂, and a second electrode 22 for measuring motion artefacts.

[0031] The circuitry 40 is configured to apply a time variable voltage V_1 to a first electrode 26 via a first operational amplifier 70, and provide a time variable signal 43 (voltage V_{out}) at an output of a second operational amplifier 80.

[0032] As illustrated in more detail in Figs 4A & 4B, the first electrode 26 and the second electrode 22 are guard electrodes for the respective first and second ECG electrodes 60₁, 60₂. The ECG electrode is centrally located. In these examples it is circular but this is not necessarily essential. The electrode 26/22 is separated from the ECG electrode 60₁/60₂, in this example, low relative permittivity gaps are used for separation.

[0033] The electrode 26/22 is a circle circumscribing but separated from the ECG electrode 60₁/60₂.

[0034] Returning to Fig 3, the ECG signal 41₁ received at the ECG electrode 60₁ is applied, via op-amp 90, as a virtual earth at a +ve terminal of a first op-amp 70. A voltage divider may be used in some examples. For example, impedances Z_A and Z_B may be connected in series between the output of the op-amp 90 and ground, and an intermediate node between impedances Z_A and Z_B may be connected to +ve terminal of the first op-amp 70.

[0035] The ECG signal 41₂ received at the ECG electrode 60₂ is applied, via op-amp 92, as a virtual earth at a +ve terminal of a second op-amp 80. A voltage divider may be used in some examples. For example, impedances Z_A' and Z_B' may be connected in series between the output of the op-amp 92 and ground, and an intermediate node between impedances Z_A' and Z_B' may be

connected to the +ve terminal of the second op-amp 80.

[0036] The first op-amp 70 generates at its output a current and a voltage V_1 at the first guard electrode 26. The first op-amp 70 is arranged for closed loop negative feedback via an impedance 72 connected between its output and its -ve terminal. The impedance 72 has a value Z_2 . The first op-amp 70 is arranged to receive an input at its -ve terminal, via an impedance 74, from a variable voltage source 76. The variable voltage source 76 produces voltage $V_{in}(t)$. The impedance 74 has a value Z_1 . The first ECG signal 41_1 received at the first ECG electrode 60_1 is applied, after amplification by op-amp 90, as a virtual earth at the +ve terminal of the first op-amp 70.

[0037] The second op-amp 80 receives at a -ve terminal a voltage from the second guard electrode 22. The second op-amp 80 is arranged for closed loop negative feedback via an impedance 82 connected between its output and its -ve terminal. The impedance 82 has a value Z_3 . The second ECG signal 41_2 received at the second ECG electrode 60_2 is applied, after amplification by op-amp 92, as a virtual earth at the +ve terminal of the second op-amp 80. The second op-amp 80 generates at its output a voltage V_{out} which is the motion artefact signal 43. In some examples, an impedance Z_4 may be connected between the second guard electrode 22 and the -ve terminal of the second op-amp 80.

[0038] The current at the -ve terminal of the second op-amp 80 depends on the voltage (V_1) at the first electrode 26 (relative to virtual earth) and an unknown impedance Z associated with the current path between the electrodes 22, 26 and through the subject's body. The impedance Z is comprised of a steady state value and a variable value that may be assumed to arise substantially from relative motion between the electrodes 22, 26 and the subject's body. The output of the op-amp 80 is therefore a variable impedance signal 43 caused by relative motion.

[0039] The current at the -ve terminal of the first op-amp 70 is V_{in}/Z_1 , where V_{in} is the variable voltage (relative to virtual earth) applied to a -ve input of the first op-amp 70 via impedance Z_1 . The first op-amp 70 is arranged for closed loop, negative feedback. The output of the first op-amp 70 is therefore $V_1 = V_{in} * (1 + Z_2/Z_1)$. The current at the -ve terminal of the second op-amp 80 is V_1/Z where V_1 is the variable voltage (relative to virtual earth) applied to a -ve input of the second op-amp 80 via the inter-electrode impedance Z . The second op-amp 80 is arranged for closed loop, negative feedback. The output of the second op-amp 80 is therefore $V_{out} = Z_3 * V_1/Z = V_{in} * (Z_3/Z) * (1 + Z_2/Z_1)$.

[0040] It is possible to separate the part of V_{out} that arises as a consequence of variation in Z from the part of V_{out} that arises as a consequence of variation in V_{in} .

[0041] This may, for example, be achieved by removing V_{in} from V_{out} in the frequency domain using a demodulator.

[0042] If Z_1, Z_2, Z_3 are resistors, then at the higher frequencies of V_{in} the steady state impedance of the body

may be considered to be primarily resistive. The changing impedance arising from the distance between the electrodes 22/26 and the skin surface will be primarily reactive (capacitive).

[0043] Changes in the imaginary (reactive) part of the variable impedance signal 43 may therefore be attributed to variation in capacitance arising from the relative motion of the electrodes 22,26 and the body. These represent motion artefacts in the sensed signal 21.

[0044] Fig 5 illustrates an example of a demodulation circuit. The demodulation circuit processes the input time-variable voltage V_{in} and the output time-variable voltage V_{out} to obtain Imaginary and Real components of the variable impedance signal 43.

[0045] The demodulation circuit may be configured to calculate how the complex transfer function between the input time-variable voltage V_{in} and the output time-variable voltage V_{out} varies over time.

[0046] Figures 6A, 6B, 6C illustrate examples of motion-associated sensors 52 configured to provide one or more motion associated signals 50. A motion-associated sensor 52 produces a motion associated signal 50 that is associated with motion of the electrode 22 of the displacement current sensor 20 relative to the user 30.

[0047] For example, as illustrated in Fig 6A, the motion associated signal 50 may be a force dependent signal that is dependent upon or responsive to a force that causes motion of the electrode 22 of the displacement current sensor 20 relative to the user 30. The motion-associated sensor 52 may, for example, be a force sensor, a pressure sensor, and/or a deformation sensor. The motion-associated sensor 52 may, for example, be an electromagnetic film sensor, a piezoelectric sensor, a strain gauge sensor.

[0048] For example, as illustrated in Fig 6B, the motion associated signal 50 may be a motion dependent signal that is dependent upon or responsive to motion of the subject's body (e.g. relative to a fixed electrode 22 of the displacement current sensor 20). The motion-associated sensor 52 may, for example, be a body wearable motion sensor. The motion-associated sensor 52 may, for example, be an accelerometer, a gyroscope, and/or a magnetometer.

[0049] For example, as illustrated in Fig 6C, the motion associated signal 50 may be a motion dependent signal that is dependent upon or responsive to motion of the electrode 22 of the displacement current sensor 20 relative to the user 30. The motion-associated sensor 52 may, for example, be a motion sensor or a distance sensor. The motion-associated sensor 52 may, for example, be a capacitive sensor, a radio frequency sensor, an ultrasound sensor, an optical sensor.

[0050] The circuitry 40 illustrated in Fig 3, produces the variable impedance signal 43 as a motion associated signal 50. The variable impedance signal 43 varies with the varying capacitance between ECG electrode 60_1 and the subject's body and ECG electrode 60_2 and the subject's body.

[0051] The motion-associated sensors 52 may be part of the apparatus 10 or separate to the apparatus 10.

[0052] The motion-associated sensor 52 may perform one of more of the sensing functions described with reference to Figs 6A to 6C.

[0053] In the example of Figs 6A to 6C, the displacement current sensor 20 is movable relative to the subject and is not affixed to the subject. For example, the electrode 22 (26) of a displacement current sensor 20 is movable relative to the subject and is not affixed to the subject.

[0054] In these examples, but not necessarily all examples, the displacement current sensor 20 is fixed to an article 56 adjacent the subject 30. The article 56 may, for example, be a bed or other furniture.

[0055] Figs 7A to 7D illustrate further examples of circuitry 40 configured to process the one or more sensed electrical signals 21 to compensate for artefacts arising from motion of the subject. The compensation for motion artefacts removes noise from the sensed electrical signal 21 producing an electrical signal 21 less affected by noise.

[0056] In the example of Fig 7A, the circuitry 40 is configured to process the sensed signal 21 to compensate for artefacts arising from motion of the subject by passing the sensed signal 21 through a band pass filter 110 configured to filter the sensed signal 21 to compensate for artefacts arising from motion of the subject 30. It may be desirable for the filter 110 to be adaptive and adapt in response to the motion associated signal 50. In some but not necessarily all examples, the filter 110 may have a fixed bandwidth or an adaptive bandwidth in the range 1-40 kHz.

[0057] In the example of Fig 7B, the circuitry 40 is configured to process the sensed signal 21 to compensate for artefacts arising from motion of the subject by:

i) determining a reliability of the sensed signal 21 over time based on the motion associated signal 50. For example, if the motion associated signal 50 indicates motion for a first period of time, then the sensed signal 21 may be flagged as unreliable for that first period of time. If the motion associated signal 50 indicates no motion for a second period of time, then the sensed signal 21 may be flagged as reliable for that second period of time.

ii) processing the sensed signal 21 using weightings based on the determined reliability. For example, if the sensed signal 21 is flagged as reliable it may have a weighting of 1 (multiplication factor=1) and if the sensed signal 21 is flagged as unreliable it may have a weighting of 0 (multiplication factor=0). It is of course possible to have weightings between 0 and 1 depending upon the degree of reliability/unreliability.

[0058] In the example of Fig 7C, the circuitry 40 is configured to process the sensed signal 21 to compensate for artefacts arising from motion of the subject by:

measuring artefacts arising from motion of the subject; and

in the frequency domain, removing the measured artefacts from the sensed signal.

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[0059] The motion associated signal 50 may be used to represent artefacts arising from motion of the subject 30. The motion associated signal 50 may be converted 112 to the frequency domain by, for example, using a transform function such as a Fourier Transform (FT). The sensed signal 21 may be converted 112 to the frequency domain by, for example, using a transform function such as a Fourier Transform (FT). A processor 116 may be used to remove the measured artefacts from the sensed signal in the frequency domain.

[0060] For example, it may be determined that the spectral components 50' of the motion associated signal 50 represent noise in the spectral components of the sensed signal 21. The spectral components of the sensed signal that correspond to the spectral components of the motion associated signal 50 may be adapted to remove motion artefacts. In some examples they may be reduced. In some examples, they may be removed.

[0061] In the example of Fig 7D, the circuitry 40 is configured to process the sensed signal 21 to compensate for artefacts arising from motion of the subject by using an adaptive filter 118 for filtering the sensed signal 21. The filtered signal or some other reference signal is used for updating the adaptive filter 118. For example, at least a part of the impedance between the first and second electrodes 60₁, 60₂ may be used as an external reference signal 117 for the adaptive filter 118 for filtering the sensed signal 21. In some but not necessarily all examples, the filter 118 may have an adaptive bandwidth in the range 1-40 kHz.

[0062] Implementation of the circuitry 40 may be as a controller 96, for example. The controller 96 may be implemented in hardware alone, have certain aspects in software including firmware alone or can be a combination of hardware and software (including firmware).

[0063] As illustrated in Fig 8 the controller 96 may be implemented using instructions that enable hardware functionality, for example, by using executable instructions of a computer program 94 in a general-purpose or special-purpose processor 90 that may be stored on a computer readable storage medium (disk, memory etc) to be executed by such a processor 90.

[0064] The processor 90 is configured to read from and write to the memory 92. The processor 90 may also comprise an output interface via which data and/or commands are output by the processor 90 and an input interface via which data and/or commands are input to the processor 90.

[0065] The memory 92 stores a computer program 94 comprising computer program instructions (computer program code) that controls the operation of the apparatus 10 when loaded into the processor 90. The computer program instructions, of the computer program 94, pro-

vide the logic and routines that enables the apparatus to perform the methods illustrated in Figs 11. The processor 90 by reading the memory 92 is able to load and execute the computer program 94.

[0066] The apparatus 10 therefore comprises:

at least one processor 90; and
 at least one memory 92 including computer program code
 the at least one memory 92 and the computer program code configured to, with the at least one processor 90, cause the apparatus 10 at least to perform:

measuring a sensed signal, from a displacement current sensor 20, dependent upon electrical activity of a subject's heart; and
 processing the sensed signal 21 to compensate for artefacts arising from motion of the subject 30.

[0067] The computer program 94 may arrive at the apparatus 10 via any suitable delivery mechanism. The delivery mechanism may be, for example, a non-transitory computer-readable storage medium, a computer program product, a memory device, a record medium such as a compact disc read-only memory (CD-ROM) or digital versatile disc (DVD), an article of manufacture that tangibly embodies the computer program 94. The delivery mechanism may be a signal configured to reliably transfer the computer program 94. The apparatus 10 may propagate or transmit the computer program 94 as a computer data signal.

[0068] Although the memory 92 is illustrated as a single component/circuitry it may be implemented as one or more separate components/circuitry some or all of which may be integrated/removable and/or may provide permanent/semi-permanent/ dynamic/cached storage.

[0069] Although the processor 90 is illustrated as a single component/circuitry it may be implemented as one or more separate components/circuitry some or all of which may be integrated/removable. The processor 90 may be a single core or multi-core processor.

[0070] References to 'computer-readable storage medium', 'computer program product', 'tangibly embodied computer program' etc. or a 'controller', 'computer', 'processor' etc. should be understood to encompass not only computers having different architectures such as single /multi-processor architectures and sequential (Von Neumann)/parallel architectures but also specialized circuits such as field-programmable gate arrays (FPGA), application specific circuits (ASIC), signal processing devices and other processing circuitry. References to computer program, instructions, code etc. should be understood to encompass software for a programmable processor or firmware such as, for example, the programmable content of a hardware device whether instructions for a processor, or configuration settings for a fixed-function device, gate array or programmable logic device etc.

[0071] As used in this application, the term 'circuitry' refers to all of the following:

- (a) hardware-only circuit implementations (such as implementations in only analog and/or digital circuitry) and
- (b) to combinations of circuits and software (and/or firmware), such as (as applicable): (i) to a combination of processor(s) or (ii) to portions of processor(s)/software (including digital signal processor(s)), software, and memory(ies) that work together to cause an apparatus, such as a mobile phone or server, to perform various functions and
- (c) to circuits, such as a microprocessor(s) or a portion of a microprocessor(s), that require software or firmware for operation, even if the software or firmware is not physically present.

This definition of 'circuitry' applies to all uses of this term in this application, including in any claims. As a further example, as used in this application, the term "circuitry" would also cover an implementation of merely a processor (or multiple processors) or portion of a processor and its (or their) accompanying software and/or firmware. The term "circuitry" would also cover, for example and if applicable to the particular claim element, a baseband integrated circuit or applications processor integrated circuit for a mobile phone or a similar integrated circuit in a server, a cellular network device, or other network device.

[0072] Fig 9 illustrates an example of a method 100 comprising:

at block 102, using a displacement current sensor 20 to measure a sensed signal 21 dependent upon electrical activity of a subject's heart;
 at block 104, processing the sensed signal 21 to compensate for artefacts arising from motion of the subject 30.

[0073] The blocks illustrated in the Figs 9 may represent steps in a method and/or sections of code in the computer program 94. The illustration of a particular order to the blocks does not necessarily imply that there is a required or preferred order for the blocks and the order and arrangement of the block may be varied. Furthermore, it may be possible for some blocks to be omitted.

[0074] Where a structural feature has been described, it may be replaced by means for performing one or more of the functions of the structural feature whether that function or those functions are explicitly or implicitly described.

[0075] As used here 'module' refers to a unit or apparatus that excludes certain parts/components that would be added by an end manufacturer or a user. The apparatus 10 may be a module.

[0076] The term 'comprise' is used in this document with an inclusive not an exclusive meaning. That is any reference to X comprising Y indicates that X may com-

prise only one Y or may comprise more than one Y. If it is intended to use 'comprise' with an exclusive meaning then it will be made clear in the context by referring to "comprising only one.." or by using "consisting".

[0077] In this brief description, reference has been made to various examples. The description of features or functions in relation to an example indicates that those features or functions are present in that example. The use of the term 'example' or 'for example' or 'may' in the text denotes, whether explicitly stated or not, that such features or functions are present in at least the described example, whether described as an example or not, and that they can be, but are not necessarily, present in some of or all other examples. Thus 'example', 'for example' or 'may' refers to a particular instance in a class of examples. A property of the instance can be a property of only that instance or a property of the class or a property of a subclass of the class that includes some but not all of the instances in the class. It is therefore implicitly disclosed that a feature described with reference to one example but not with reference to another example, can where possible be used in that other example but does not necessarily have to be used in that other example.

[0078] Although embodiments of the present invention have been described in the preceding paragraphs with reference to various examples, it should be appreciated that modifications to the examples given can be made without departing from the scope of the invention as claimed.

[0079] Features described in the preceding description may be used in combinations other than the combinations explicitly described.

[0080] Although functions have been described with reference to certain features, those functions may be performable by other features whether described or not.

[0081] Although features have been described with reference to certain embodiments, those features may also be present in other embodiments whether described or not.

[0082] Whilst endeavoring in the foregoing specification to draw attention to those features of the invention believed to be of particular importance it should be understood that the Applicant claims protection in respect of any patentable feature or combination of features hereinbefore referred to and/or shown in the drawings whether or not particular emphasis has been placed thereon.

Claims

1. An apparatus comprising:

a displacement current sensor configured to measure a sensed signal dependent upon electrical activity of a subject's heart; and
 circuitry configured to process the sensed signal to compensate for artefacts arising from motion of the subject.

2. An apparatus as claimed in claim 1, wherein the displacement current sensor comprises at least one electrode adjacent the subject's skin and comprising electrical insulation for insulating the at least one electrode from the subject's skin.

3. An apparatus as claimed in claim 2, wherein the at least one electrode is movable relative to the subject and is not affixed to the subject.

4. An apparatus as claimed in claim 3, wherein the at least one electrode is embedded in a bed or other furniture.

5. An apparatus as claimed in any preceding claim, wherein the circuitry is configured to process the sensed signal to compensate for artefacts arising from motion of the subject, to provide an ECG signal.

6. An apparatus as claimed in any preceding claim, wherein the apparatus comprises a sensor for detecting motion of the subject and/or a sensor for detecting pressure or force between the subject and the displacement current sensor.

7. An apparatus as claimed in any preceding claim, wherein the circuitry configured to process the sensed signal to compensate for artefacts arising from motion of the subject comprises:

a band pass filter for filtering the sensed signal to compensate for artefacts arising from motion of the subject.

8. An apparatus as claimed in any preceding claim, wherein the circuitry configured to process the sensed signal to compensate for artefacts arising from motion of the subject is configured to:

determine reliability of the sensed signal over time based on motion of the subject, and process the sensed signal using weightings based on the determined reliability.

9. An apparatus as claimed in any preceding claim, wherein the circuitry configured to process the sensed signal to compensate for artefacts arising from motion of the subject is configured to:

measure artefacts arising from motion of the subject; and
 in the frequency domain, remove the measured artefacts from the sensed signal.

10. An apparatus as claimed in any preceding claim, wherein the circuitry configured to process the sensed signal to compensate for artefacts arising from motion of the subject comprises: 5
- an adaptive filter for filtering the sensed signal.
11. An apparatus as claimed in any preceding claim, wherein the apparatus comprises a first electrode and a second electrode; and the circuitry configured to process the sensed signal to compensate for artefacts arising from motion of the subject is configured to apply a reference signal to the first electrode and to sense at the second electrode an additional signal dependent upon motion of the subject and to use the additional signal to process the sensed signal to compensate for artefacts arising from motion of the subject. 10
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12. An apparatus as claimed in claim 11, wherein the circuitry configured to process the sensed signal to compensate for artefacts arising from motion of the subject is configured to apply a first time variable voltage to the first electrode via a first operational amplifier, measure a second time variable voltage at an output of a second operational amplifier wherein an input to the second operational amplifier is connected to the second electrode, an impedance being connected between the input and the output of the second operational amplifier, wherein at least a part of the impedance between the first and second electrodes is estimated using at least the first time variable voltage and the second time variable voltage to estimate motion of the subject. 25
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13. An apparatus as claimed in claim 12, wherein the first operational amplifier is virtually earthed by an ECG signal received at a first ECG electrode adjacent the first electrode and guarded by the first electrode and the second operational amplifier is virtually earthed by an ECG signal received at a second ECG electrode adjacent the second electrode and guarded by the second electrode. 40
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14. An apparatus as claimed in claim 12 or 13, configured to use at least a part of the impedance between the first and second electrodes as an external reference signal for an adaptive filter for filtering the sensed signal. 50
15. A method comprising:
- using a displacement current sensor to measure a sensed signal dependent upon electrical activity of a subject's heart; 55
processing the sensed signal to compensate for artefacts arising from motion of the subject.

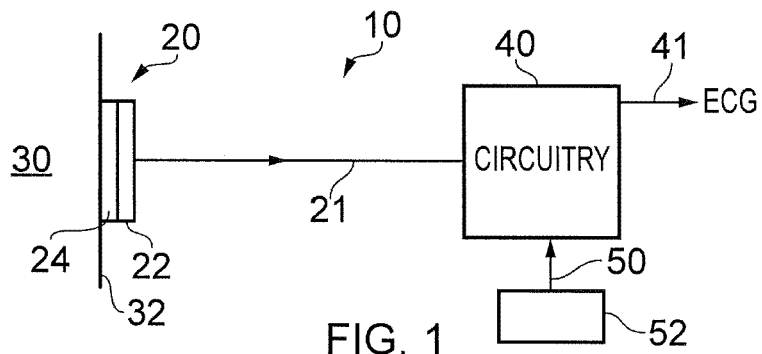


FIG. 1

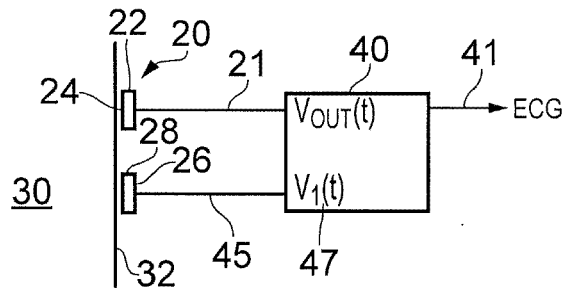


FIG. 2

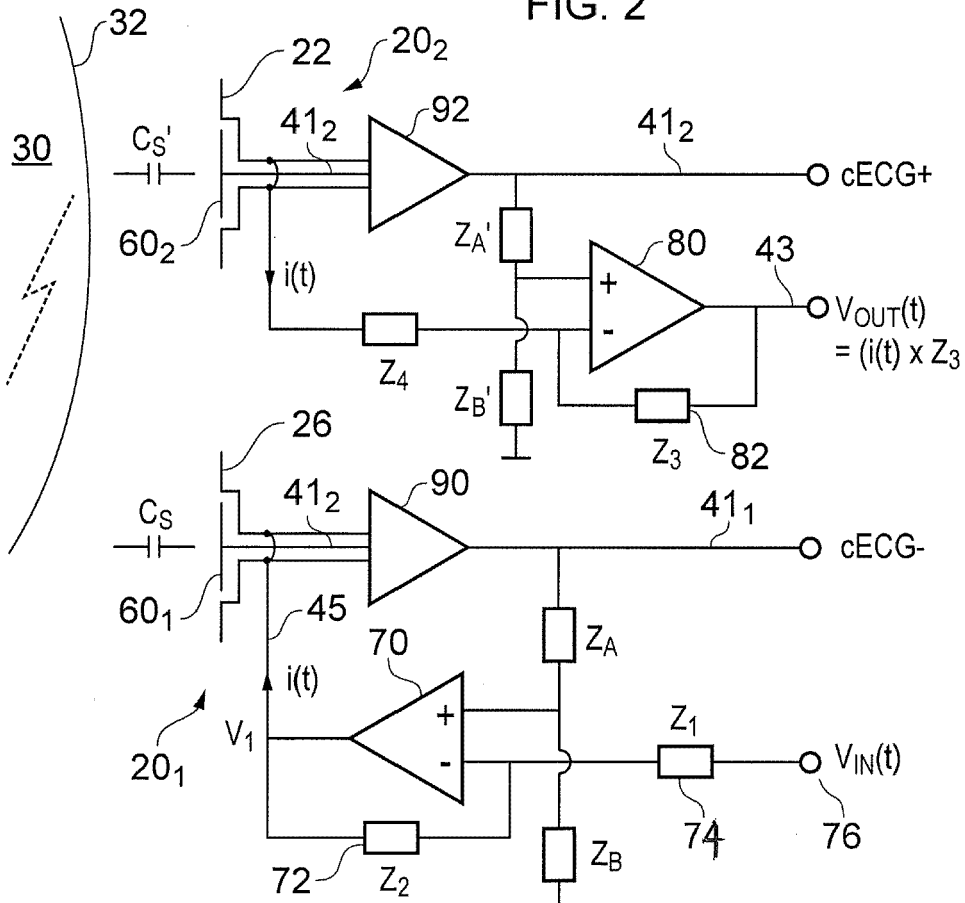


FIG. 3

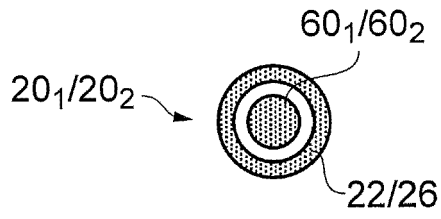


FIG. 4A

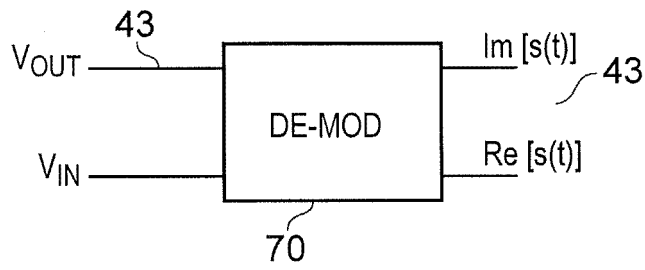


FIG. 5

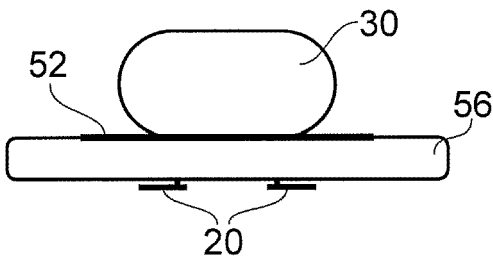


FIG. 6A

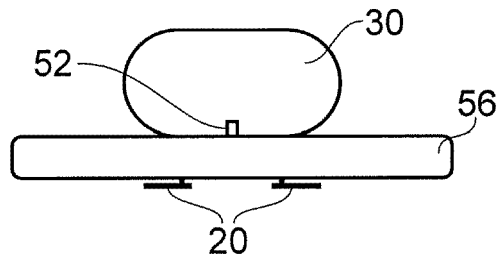


FIG. 6B

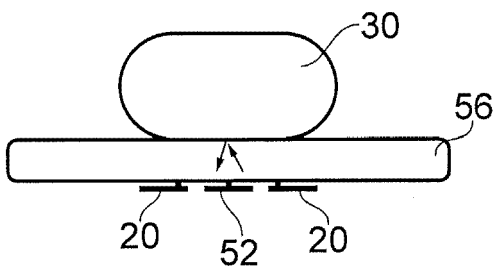


FIG. 6C

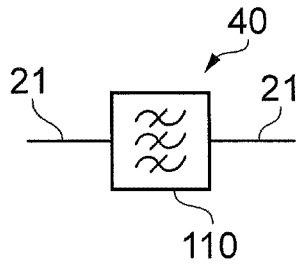


FIG. 7A

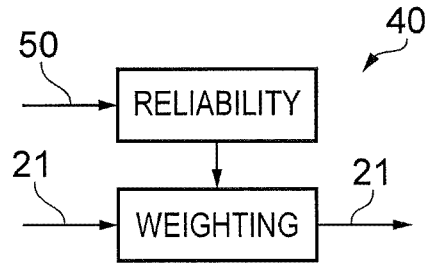


FIG. 7B

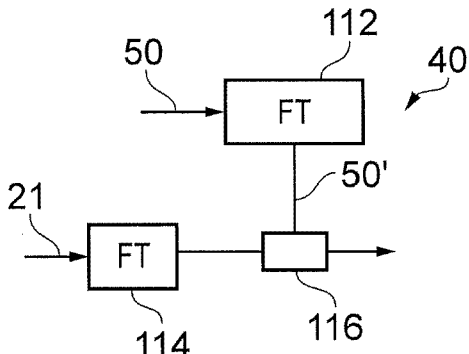


FIG. 7C

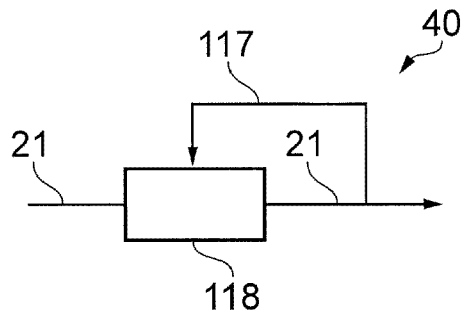


FIG. 7D

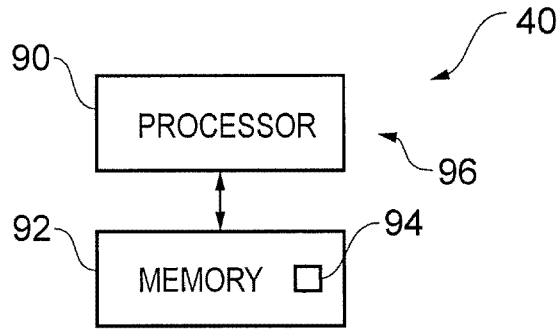


FIG. 8

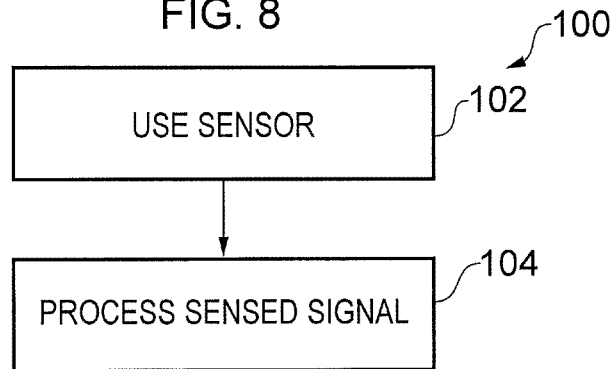


FIG. 9



EUROPEAN SEARCH REPORT

Application Number
EP 17 20 3659

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DOCUMENTS CONSIDERED TO BE RELEVANT			
Category	Citation of document with indication, where appropriate, of relevant passages	Relevant to claim	CLASSIFICATION OF THE APPLICATION (IPC)
X	SERTEYN A ET AL: "Motion Artifacts in Capacitive ECG Measurements: Reducing the Combined Effect of DC Voltages and Capacitance Changes Using an Injection Signal", IEEE TRANSACTIONS ON BIOMEDICAL ENGINEERING, IEEE SERVICE CENTER, PISCATAWAY, NJ, USA, vol. 62, no. 1, 1 January 2015 (2015-01-01), pages 264-273, XP011568272, ISSN: 0018-9294, DOI: 10.1109/TBME.2014.2348178 [retrieved on 2014-12-18] * figures 1-5, 9, 11-15 * * abstract * * Parts II-IV, VI-X *	1-10,15	INV. A61B5/00 A61B5/0428 G01R19/25 A61B5/0402
X	SERTEYN ALINE ET AL: "Using an injection signal to reduce motion artifacts in capacitive ECG measurements", ENGINEERING IN MEDICINE AND BIOLOGY SOCIETY (EMBC), 2013 35TH ANNUAL INTERNATIONAL CONFERENCE OF THE IEEE, IEEE, 3 July 2013 (2013-07-03), pages 4795-4798, XP032489259, ISSN: 1557-170X, DOI: 10.1109/EMBC.2013.6610620 [retrieved on 2013-09-25] * figures 1-6 * * Parts II, III, IV, V, VI *	1,5-7,9,10,15	TECHNICAL FIELDS SEARCHED (IPC) A61B G01R

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The present search report has been drawn up for all claims			
Place of search The Hague		Date of completion of the search 16 May 2018	Examiner Knoop, Jan
CATEGORY OF CITED DOCUMENTS X : particularly relevant if taken alone Y : particularly relevant if combined with another document of the same category A : technological background O : non-written disclosure P : intermediate document		T : theory or principle underlying the invention E : earlier patent document, but published on, or after the filing date D : document cited in the application L : document cited for other reasons ----- & : member of the same patent family, corresponding document	

6 EPO FORM 1503 03.02 (P04C01)



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Application Number
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DOCUMENTS CONSIDERED TO BE RELEVANT			
Category	Citation of document with indication, where appropriate, of relevant passages	Relevant to claim	CLASSIFICATION OF THE APPLICATION (IPC)
X	EP 3 050 501 A1 (NISSAN MOTOR [JP]; UNIV TOKYO DENKI [JP]) 3 August 2016 (2016-08-03) * figures 1-3 * * paragraph [0010] - paragraph [0037] * * paragraph [0098] * * paragraph [0105] - paragraph [0108] *	1-5,7-15	
X	EP 2 294 979 A1 (IMEC [BE]) 16 March 2011 (2011-03-16) * figures 4, 8 * * paragraph [0021] - paragraph [0037] * * paragraph [0044] - paragraph [0045] *	1-5,7,9-15	
			TECHNICAL FIELDS SEARCHED (IPC)
The present search report has been drawn up for all claims			
Place of search The Hague		Date of completion of the search 16 May 2018	Examiner Knoop, Jan
CATEGORY OF CITED DOCUMENTS X : particularly relevant if taken alone Y : particularly relevant if combined with another document of the same category A : technological background O : non-written disclosure P : intermediate document		T : theory or principle underlying the invention E : earlier patent document, but published on, or after the filing date D : document cited in the application L : document cited for other reasons & : member of the same patent family, corresponding document	

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**ANNEX TO THE EUROPEAN SEARCH REPORT
ON EUROPEAN PATENT APPLICATION NO.**

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5 This annex lists the patent family members relating to the patent documents cited in the above-mentioned European search report.
The members are as contained in the European Patent Office EDP file on
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16-05-2018

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For more details about this annex : see Official Journal of the European Patent Office, No. 12/82

专利名称(译)	生物信号检测		
公开(公告)号	EP3488767A1	公开(公告)日	2019-05-29
申请号	EP2017203659	申请日	2017-11-24
[标]申请(专利权)人(译)	诺基亚技术有限公司		
申请(专利权)人(译)	NOKIA TECHNOLOGIES OY		
当前申请(专利权)人(译)	NOKIA TECHNOLOGIES OY		
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IPC分类号	A61B5/00 A61B5/0428 G01R19/25 A61B5/0402		
CPC分类号	A61B5/04284 A61B5/6891 A61B5/721 A61B2560/0468 A61B2562/0214		
外部链接	Espacenet		

摘要(译)

一种装置，包括：位移电流传感器，被配置为根据受试者心脏的电活动测量感测信号；和电路，被配置为处理所感测的信号以补偿由对象的运动引起的假象。

