



(12) **EUROPEAN PATENT APPLICATION**

(43) Date of publication:  
**22.11.2017 Bulletin 2017/47**

(51) Int Cl.:  
**A61B 5/00 (2006.01) A61B 5/08 (2006.01)**  
**A61M 16/00 (2006.01) A61M 16/16 (2006.01)**  
**A61M 16/10 (2006.01)**

(21) Application number: **17171378.7**

(22) Date of filing: **07.11.2012**

(84) Designated Contracting States:  
**AL AT BE BG CH CY CZ DE DK EE ES FI FR GB GR HR HU IE IS IT LI LT LU LV MC MK MT NL NO PL PT RO RS SE SI SK SM TR**

- **FARRUGIA, Steven Paul**  
**Bella Vista, New South Wales 2153 (AU)**
- **DENNIS, Clancy John**  
**Bella Vista, New South Wales 2153 (AU)**
- **BERTHON-JONES, Michael**  
**Bella Vista, New South Wales 2153 (AU)**
- **BASSIN, David John**  
**Bella Vista, New South Wales 2153 (AU)**
- **TESCHLER, Helmut**  
**42553 Velbert (DE)**

(30) Priority: **07.11.2011 AU 2011904599**  
**15.06.2012 AU 2012902501**  
**26.06.2012 AU 2012902693**

(62) Document number(s) of the earlier application(s) in accordance with Art. 76 EPC:  
**12846933.5 / 2 776 101**

(74) Representative: **Vossius & Partner**  
**Patentanwälte Rechtsanwälte mbB**  
**Siebertstrasse 3**  
**81675 München (DE)**

(71) Applicant: **ResMed Limited**  
**Bella Vista, NSW 2153 (AU)**

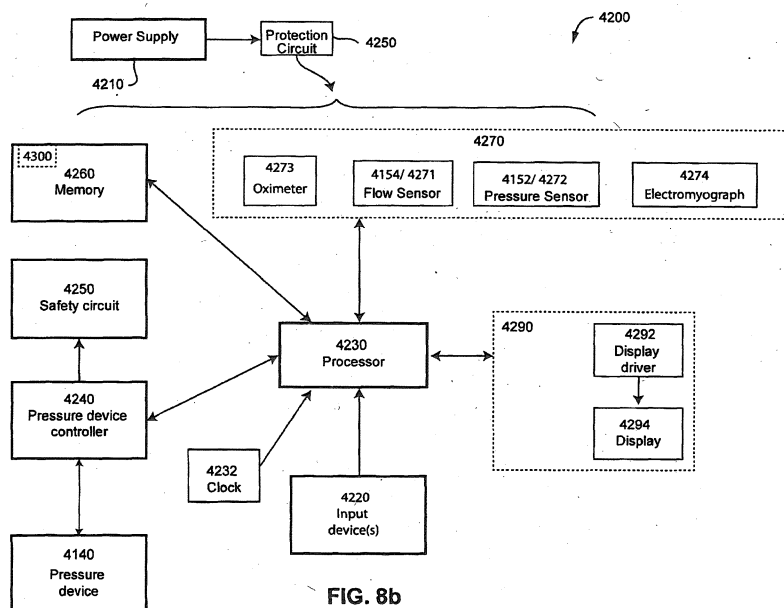
(72) Inventors:  
 • **SCHINDHELM, Klaus Henry**  
**Bella Vista, New South Wales 2153 (AU)**  
 • **MALOUF, Gordon Joseph**  
**Bella Vista, New South Wales 2153 (AU)**

Remarks:

This application was filed on 16-05-2017 as a divisional application to the application mentioned under INID code 62.

(54) **APPARATUS FOR PROVIDING VENTILATION TO A PATIENT**

(57) The present technology relates an apparatus to provide ventilation to patients. In particular, the present technology relates to changing ventilator parameters to match changing patient metabolic demand.



**FIG. 8b**

## Description

### 1 CROSS-REFERENCE TO RELATED APPLICATIONS

[0001] This patent application claims the benefit of priority to Australian Provisional Patent Applications AU 2011904599 filed 7 November 2011, AU 2012902501 filed 15 June 2012 and AU 2012902693 filed 26 June 2012, the entire contents of each being incorporated herein by reference.

### 2 BACKGROUND OF THE INVENTION

#### 2.1 FIELD OF THE INVENTION

[0002] The present technology relates to methods and apparatus for the treatment and/or amelioration of respiratory disorders. In particular, the present technology relates to methods and apparatus for providing ventilation to a patient.

#### 2.2 RELATED ART

[0003] The respiratory system of the body facilitates gas exchange. The nose and mouth form the entrance to the airways of a patient.

[0004] The airways consist of a series of branching tubes, which become narrower, shorter and more numerous as they penetrate deeper into the lung. The prime function of the lung is gas exchange, allowing oxygen to move from the air into the venous blood and carbon dioxide to move out. The trachea divides into right and left main bronchi, which further divide eventually into terminal bronchioles. The bronchi make up the conducting airways, and do not take part in gas exchange. Further divisions of the airways lead to the respiratory bronchioles, and eventually to the alveoli. The alveolated region of the lung is where the gas exchange takes place, and is referred to as the respiratory zone. See West, Respiratory Physiology- the essentials.

[0005] A range of respiratory disorders exist.

[0006] Chronic Obstructive Pulmonary Disease (COPD) encompasses any of a group of lower airway diseases that have certain characteristics in common. These include increased resistance to air movement, extended expiratory phase of respiration, and loss of the normal elasticity of the lung. Examples of COPD are emphysema and chronic bronchitis. COPD is caused by chronic tobacco smoking (primary risk factor), occupational exposures, air pollution and genetic factors. Symptoms include: dyspnoea on exertion, chronic cough and sputum production.

[0007] Neuromuscular Disease (NMD) is a broad term that encompasses many diseases and ailments that impair the functioning of the muscles either directly via intrinsic muscle pathology, or indirectly via nerve pathology. Some NMD patients are characterised by progressive

muscular impairment leading to loss of ambulation, being wheelchair-bound, swallowing difficulties, respiratory muscle weakness and, eventually, death from respiratory failure. Neuromuscular disorders can be divided into rapidly progressive and slowly progressive: (i) Rapidly progressive disorders: Characterised by muscle impairment that worsens over months and results in death within a few years (e.g. Amyotrophic lateral sclerosis (ALS) and Duchenne muscular dystrophy (DMD) in teenagers); (ii) Variable or slowly progressive disorders: Characterised by muscle impairment that worsens over years and only mildly reduces life expectancy (e.g. Limb girdle, Facio-scapulohumeral and Myotonic muscular dystrophy). Symptoms of respiratory failure in NMD include: increasing generalised weakness, dysphagia, dyspnoea on exertion and at rest, fatigue, sleepiness, morning headache, and difficulties with concentration and mood changes.

[0008] Chest wall disorders are a group of thoracic deformities that result in inefficient coupling between the respiratory muscles and the thoracic cage. The disorders are usually characterised by a restrictive defect and share the potential of long term hypercapnic respiratory failure. Scoliosis and/or kyphoscoliosis may cause severe respiratory failure. Symptoms of respiratory failure include: dyspnoea on exertion, peripheral oedema, orthopnoea, repeated chest infections, morning headaches, fatigue, poor sleep quality and loss of appetite.

[0009] Mechanical ventilators have been used to ameliorate the above respiratory disorders.

### 3 SUMMARY

[0010] The present technology relates to providing ventilation and, in particular, to methods and apparatus for providing ventilation to awake patients.

[0011] The present technology also relates to methods and apparatus providing ventilation to sleeping patients.

[0012] One aspect of one form of the present technology is a method of providing ventilatory support, or ventilatory assistance, to assist a patient to exercise.

[0013] One aspect of one form of the present technology is a ventilator constructed and arranged to assist a patient to exercise.

[0014] Another aspect of one form of the present technology is a ventilator constructed and arranged to reduce a ventilatory limitation to exercise as the result of disease.

[0015] An aspect of one form of the present technology is a ventilator that is responsive the rate of respiration of a patient.

[0016] Another aspect of one form of the present technology relates to methods and apparatus for improving the comfort of awake patients being provided with non-invasive ventilation.

[0017] Another aspect of one form of the present technology relates to methods and apparatus for changing ventilation parameters of a ventilator to match patient metabolic demand, in particular when the metabolic de-

mand is changing. In one form the present technology provides an increase to either or both of ventilation and ventilatory support as metabolic load increases.

**[0018]** Another aspect of one form of the present technology is a ventilator that is configurable to move between a plurality of different settings to assist a patient in an exercise regime, as metabolic demand increases, and/or as metabolic demand decreases.

**[0019]** One aspect of one form of the present technology is a processor programmed to implement one or more algorithms.

**[0020]** Another aspect of one form of the present technology relates to a ventilator having a plurality of predefined discrete activity modes or states and moves manually or automatically between modes or states (e.g. (i) Quiet sitting; (ii) Walking around; (iii) Running). In another form, the ventilator has a predefined continuous support pathway, and moves (manually or automatically) along the pathway in response to demand. In this way, an indication of change in metabolic demand and/or lung mechanics is input manually or automatically. Preferably the modes or pathway will have an Expiratory Positive Air Pressure (EPAP) value that ranges from about 4cmH<sub>2</sub>O to a limit of about 10cmH<sub>2</sub>O. In one form the limit is a predetermined limit. In other forms, the limit is not predetermined and is calculated from a measure of intrinsic PEEP. At this limit, an additional increase, or further increases in demand preferably do not give rise to a further increase in EPAP, hence the level of expiratory positive air pressure will remain substantially constant. Manual adjustments may be made using a remote control, e.g. with buttons and/or joystick.

**[0021]** Another aspect of the present technology relates to apparatus that allows a patient to manually trigger a ventilator to deliver a breath. In particular, the present technology may allow a patient to manually trigger delivery by the ventilator of an inspiration phase of a breath to the patient.

**[0022]** Another aspect of the present technology relates to apparatus that allows a patient to manually cycle a ventilator, and thus to manually cause the device to transition from the inspiratory phase to the exhalation phase. Breaths may be cycled by a mechanical ventilator when a set time has been reached, or when a pre-set flow or percentage of the maximum flow delivered during a breath is reached, depending on the breath type and the settings. Here, preferably breaths can be manually cycled upon a manual cycle command given by a patient.

**[0023]** Another aspect of the present technology relates to apparatus that allows a patient to manually adjust the level of pressure support or the target ventilation of a ventilator.

**[0024]** Another aspect of the present technology relates to apparatus that allows a patient to manually adjust the level of End Expiratory Pressure (EEP) or Expiratory Positive Air Pressure (EPAP) of a ventilator.

**[0025]** Another aspect of one form of the present technology relates to a controller for a ventilator constructed

and arranged to calculate a typical duration of a manually triggered breath or a manually cycled breath.

**[0026]** Another aspect of one form of the present technology relates to methods and apparatus that, in a first mode, allow a patient to manually control one or more of the following features; triggering, cycling, the level of pressure support, EEP, or EPAP and the level of target ventilation. In a second mode, the apparatus may provide one or more of automatic triggering, cycling or automatically adjusting the level of pressure support, EEP, or EPAP and the level of target ventilation. In some instances, the automatic adjustments may be based, at least in part, on data obtained from the manual triggering, cycling, target ventilation and/or pressure support level established by the patient.

**[0027]** According to one form of the present technology, a portable battery powered ventilator is provided. In one form the ventilator comprises one or more manual controls constructed and arranged to allow the patient to adjust a ventilator setting between different modes or states, with at least some states being associated with different activity or exercise levels. Alternatively or additionally, the ventilator is constructed and arranged to automatically adjust to different activity or exercise levels of the patient

**[0028]** In one form of the present technology, a controller for a ventilator is provided, the ventilator being configured to deliver a pressure support waveform to a patient, said pressure support waveform having an inspiratory phase and a subsequent expiratory phase, and the controller being configured to trigger adjustment of at least one parameter of the ventilator in response to indication of a change in metabolic demand and/or lung mechanics of the patient.

**[0029]** In one form, a controller is programmed so that a magnitude of change to the pressure during the expiratory phase is equal to about one third of a magnitude of change during the inspiratory phase.

**[0030]** Preferably the controller is further configured to accept a signal from a metabolic demand responsive transducer, and to determine a state of metabolic demand from said metabolic demand responsive transducer. A metabolic demand responsive transducer may be one or more of an oximeter, a flow sensor and an electromyograph, e.g. a diaphragm electromyograph.

**[0031]** The following further aspects are preferred forms of the present technology.

1. A controller for a ventilator configured to allow a patient to manually trigger a breath.
2. A controller for a ventilator configured, preferably according to any one of the previous aspects, to allow a patient to manually cycle a breath.
3. A controller for a ventilator, preferably according to any one of the previous aspects, constructed and arranged to calculate a typical duration of a manually

triggered breath.

4. A controller for a ventilator, preferably according to any one of the previous aspects, constructed and arranged to calculate a typical duration of a manually cycled breath.

5. A controller for a ventilator, preferably according to any one of the previous aspects, constructed and arranged to automatically trigger to deliver a first breath and to trigger to deliver a subsequent breath after the elapse of a time duration calculated from a duration of at least one manually triggered breath.

6. A controller for a ventilator, preferably according to any one of the previous aspects, constructed and arranged to automatically cycle to stop delivery of a first breath and to cycle to stop delivery of a subsequent breath after the elapse of a time duration calculated from a duration of at least one manually cycled breath.

7. A controller for a ventilator, preferably according to any one of the previous aspects, the controller being configured to allow a patient to manually adjust at least one of the following; a target pressure support, a target ventilation level, IPAP, EPAP, a backup rate, Ti min. and Ti max.

8. A controller, preferably according to any one of the previous aspects, configured to change one of IPAP or EPAP, in response of a change in the other one.

9. The controller of aspect 8, wherein the change in the respective one of the IPAP and EPAP, the change being a response to a change in the other one, is based on a predetermined function.

10. A controller for a ventilator, preferably according to any one of the previous aspects, the controller being configured to; receive signals indicative of level of movement of the patient; and in response to the indicated level of movement, automatically adjust at least one of the following; a target pressure support, a target ventilation level, IPAP, EPAP, a backup rate, Ti min. and Ti max provided to the patient.

11. A controller for a ventilator, preferably according to any one of the previous aspects, the controller being configured to; receive signals indicative of the speed of movement of the patient; and in response to the indicated speed, automatically adjust at least one of the following; a target pressure support, a target ventilation level, IPAP, EPAP, a backup rate, Ti min. and Ti max provided to the patient.

12. A controller for a ventilator, preferably according

to any one of the previous aspects, the controller being configured to; receive signals indicative of heart rate of respiration rate of the patient; and in response to the indicated heart rate of respiration rate, automatically adjust at least one of the following; a target pressure support, a target ventilation level, IPAP, EPAP, a backup rate, Ti min. and Ti max provided to the patient.

13. A ventilator comprising the controller of any one of the preceding aspects.

14. The ventilator of aspect 13, the ventilator further comprising a manual controller in communication with the ventilator controller, the manual controller being configured to initiate a manual adjustment of at least one of the following; a target pressure support, a target ventilation level, IPAP, EPAP, a backup rate, Ti min. and Ti max provided to the patient.

15. A ventilator, preferably according to any one of the previous aspects, constructed and arranged to be adaptable to changing patient metabolic demand.

#### 4 BRIEF DESCRIPTION OF FIGURES

##### [0032]

Figure 1 shows apparatus including a push-button, a personal computer and a ventilator in accordance with an aspect of the present technology.

Figures 2a and 2b show graphs of pressure (y-axis) provided to a patient, versus time (x-axis) in accordance with an aspect of the present technology and a window in which manual triggering is available. Figure 2a shows an arbitrary triggering window during an EPAP phase (e.g. an expiratory pressure phase in a pressure waveform provided by a ventilator), in which the patient is free to manually trigger a breath, but in this case, does not manually trigger within the window. In the illustrated form, the window is about 1 second long, although in other forms it may be of a different size. By way of contrast, in Fig. 2b, the patient has initiated early manual triggering.

Figures 3a and 3b shows a graph of pressure (y-axis) versus time (x-axis) in accordance with an aspect of the present technology in which manual cycling is available. Figure 3a shows an arbitrary cycling window during an Inspiratory Positive Airway Pressure (IPAP) phase in which the patient is free to manually cycle the ventilator, but in this case, the patient does not manually cycle the ventilator. In the illustrated form, the window is about 1.8 second long, although in other forms it may be a different size. By way of contrast, in Fig. 3b, the patient has initiated early manual cycling.

Figure 4 shows a schematic of flow versus time for a spontaneously breathing patient exhibited through inspiration and expiration cycles of a breathing cycle. A detail of a portion of the breath is shown in Fig. 5.

Figure 5 shows a detail of Fig. 4. In particular, the Figure shows a portion of a breath with two time points, namely the point in time when a button trigger was manually activated ("button trigger") and the time point when the ventilator would have automatically triggered as flow would have exceeded a trigger flow point, ("Standard trigger flow").

Figure 6 illustrates over time pressure, and activation status of a trigger button and a cruise-control button.

Figures 7A and 7B show exemplary options of a pathway in accordance with one aspect of the present technology. The X-axis is metabolic demand, and the Y-axis is pressure. In Figs. 7A and 7B, two lines are shown, an EPAP line, and an IPAP line. The level of pressure support at a given level of metabolic demand is the difference between the two lines. As the level of metabolic demand increases, both EPAP and IPAP may increase, e.g. at different rates. Hence the level of support may increase from about 7cmH<sub>2</sub>O when demand is low, to about 15cmH<sub>2</sub>O when demand is high. An EPAPmax limit is defined. As metabolic demand increases, EPAP may increase to a maximum level of EPAPmax, and a further increase in metabolic demand may give rise to a further increase in IPAP, but not to EPAP. The value of EPAPmax may vary from patient to patient. In one form EPAPmax is about 10cmH<sub>2</sub>O. In Fig. 7A, the EPAP and IPAP lines are reflective of a continuous change in values in response to changes in demand, however, in an alternative form exemplarily seen in Fig. 7B, there may be discrete changes, hence the lines resemble steps.

Fig. 8a shows a Positive Airway Pressure (PAP) device in accordance with one form of the present technology.

Fig. 8b shows a schematic diagram of electric components for a PAP device in accordance with one form of the present technology.

Fig. 9 shows, in accordance with one form of the present technology, a PAP device connected to a humidifier, providing a supply of air via an air circuit to a patient interface that is being worn by a patient. As depicted, the patient may be sitting quietly reading a book prior to exercising.

Fig. 10 shows an alternative form of one aspect of the present technology.

Fig. 11 shows an example flowchart for implementing control of treatment in some aspects of the present technology.

- 5 **[0033]** The patient may move the ventilator between different stages or states of demand manually, e.g. by pressing buttons on a remote control. In another form, the ventilator will automatically detect a change in demand e.g. by monitoring one or more of heart rate, breathing (or respiratory) rate, and movement.

## 5 DETAILED DESCRIPTION

- 10 **[0034]** Some patients with certain forms of cardio-respiratory disease, for example COPD or kyphoscoliosis, may benefit from exercise, but find it difficult to exercise. The use of a ventilator may assist the patient to perform exercise, when the ventilator performs at least some of the work of breathing. Should the patient's level of activity change (and corresponding metabolic demand), then a set of ventilator parameters (e.g. level of support, timing of breaths) that might have been appropriate for the first level of activity may be inappropriate for a second level of activity, for example when a patient is becoming more active, or when becoming less active.

- 20 **[0035]** According to one aspect of the present technology, an apparatus 10 is provided as shown in Fig. 1. The apparatus 10 comprises:

30 A ventilator device 12, for example a Positive Airway Pressure (PAP) ventilator device, further for example a RESMED STELLAR® ventilator;

35 A user input device or control member, preferably a push-button 14, preferably connectable to other devices such as a personal computer via a Universal Serial Bus (USB); and

40 A controller or a Personal Computer (PC) 16 running a manual triggering and/or cycling application.

- 45 **[0036]** In certain forms of the present technology, the Positive Airway Pressure (PAP) device may be in the form of a device 4000 (see, e.g., Figs. 8a and 9) that includes an embedded processor 4230 (see, e.g., in Fig. 8b) for executing one or more algorithms that are stored in a memory 4260. This embedded processor 4230 may be provided instead or in addition to the processor existing in the Personal Computer 16 in apparatus 10. In the description hereinbelow where reference is made only to one of the devices 16,4230 or 12,4000 it should be understood that same may be applicable also to the other device 16,4230 or 12,4000 not mentioned.

### 55 5.1 Systems, Algorithms and Processes

- [0037]** An aspect of the present technology is one or more algorithms 4300 that may be executed by a con-

troller 16 or a processor 4230. In the accompanying figures algorithm 4300 is indicated in Fig. 8b as being executed by processor 4230; however it is to be understood that algorithm 4300 may also accordingly be executed by controller 16.

### 5.1.1 PATIENT INTERVENTION

#### 5.1.1.1 Triggering and cycling

**[0038]** In this embodiment, the apparatus 10 is programmed and configured so that pressing the button 14 down will trigger the ventilator 12 and releasing the button 14 will cause the ventilator 12 to cycle. The inventors have found that this configuration of push to trigger and release to cycle is easy to use.

**[0039]** In an alternative configuration, there may be different trigger and cycle buttons or different trigger and cycle activators.

**[0040]** In one form, the normal spontaneous triggering and cycling operation is unaffected.

**[0041]** In one form, the successful button-initiated triggering and cycling are subject to certain timing window limits.

**[0042]** In this form, a digital communication interface 18 of the ventilator, preferably a ResMed STELLAR® ventilator, that allows for remote control of settings is used, similar to that used in a sleep laboratory environment. A controller, such as a PC application, monitors the push-button state and sends the appropriate setting changes to the ventilator 12; temporarily changing the parameter "Backup Rate" in the case of triggering and the parameter "TiMax" for cycling.

**[0043]** "Backup Rate", with units of breaths per minute, is a preferred parameter of the ventilator 12 that establishes the minimum number of breaths per minute that the ventilator 12 will deliver, if not otherwise triggered. This parameter may be used to virtually instantaneously trigger a breath. This is so because, if the ventilator 12 is currently in expiration, increasing substantially the Backup Rate reduces the duration of the expiration cycle and effectively triggers a subsequent breath.

**[0044]** "TiMax", with units of time, is a preferred parameter of the ventilator 12 indicative of, the maximum time, from the commencement of a first breath, before the ventilator 12 will automatically change to expiration, if not otherwise cycled. If the ventilator 12 is currently in inspiration, then setting the TiMax to be very short can force a cycle (from inspiration to expiration) in a manner similar to the way an increased backup rate forces a trigger.

**[0045]** A particularity of the ventilator 12 preferably used with this technology, preferably a ResMed STELLAR ventilator, is that the allowable settings of TiMax may be determined by the current setting of Backup Rate.

**[0046]** In the embodiments shown in Figs. 2a, 2b and Figs. 3a, 3b; the, preferably STELLAR, ventilator 12 is configured as follows:

For a patient breathing at a nominal 30 breaths per minute (BPM):

Mode: S (i.e. "Spontaneous" mode for detecting a spontaneous breath of a patient)

Backup Rate: 15 BPM

TiMax:2.0sec

#### 5.1.1.2 Manual Triggering

**[0047]** The apparatus is further configured so that upon manual activation of the trigger button the apparatus implements the following steps:

(i) Set Backup Rate to 60 BPM (this has the side-effect of changing the TiMax to 0.8sec)

(ii) Wait 15ms

(iii) Set Backup Rate back to 15 BPM

(iv) Set TiMax back to 2.0sec

**[0048]** In one form of the present technology, manual triggering of a breath is only possible during an EPAP phase, and/or during a defined portion of the EPAP phase.

**[0049]** However it is noted that in other forms of the present technology, other settings may be used.

#### 5.1.1.3 Manual Cycling

**[0050]** The apparatus is further configured so that upon manual activation of the cycle button the apparatus implements the following steps:

(i) Set Backup Rate to 60 BPM (this allows  $0.2 < \text{TiMax} < 0.8$ )

(ii) Set TiMax to 0.3sec

(iii) Wait 15ms

(iv) Set Backup Rate back to 15 BPM

(v) Set TiMax back to 2.0sec

**[0051]** With reference to Fig. 2a and 2b, the following exemplary scenarios are illustrated. A patient progresses through one or more breaths (one being shown). With the ventilator 12 set to a TiMax of 2 seconds, the next breath will not be delivered until the elapse of 2 seconds. In the illustrated example (see Fig. 2b), the patient manually triggers the ventilator 12 before the elapse of the 2 seconds, and thereupon the next breath will be delivered to the patient. Manually triggering the ventilator may be

possible in this example within an "arbitrary triggering window" of 1 second that is indicated in these figures. An exemplary beginning of a next breath that is early manually triggered during this window is indicated in figure 2b by a dashed line.

**[0052]** In an embodiment, this is achieved by increasing the backup rate to a rate that is much faster than a normal rate, for example from 15 BPM to 60 BPM. At this relatively rapid rate, a new breath (indicated accordingly by the dashed line) will be soon delivered. However shortly thereafter, e.g. 15ms later, the backup rate will be returned to a lower level, e.g. a previous lower level of 15 BPM.

**[0053]** With reference to Figs. 3a and 3b, in the midst of the ventilator 12 delivering a breath to the patient, the patient activates manual cycling- for example by releasing a button- whereupon the ventilator 12 stops delivering the breath.

**[0054]** In the illustrated embodiment, TiMax is set to e.g. 0.2sec, a duration that is soon passed, and therefore the ventilator 12 may stop delivering the breath as indicated by the dashed lines in figure 3b. Here too there is an "arbitrary cycling window" during the IPAP phase in which the patient is able to manually cycle the ventilator. In these figures, the window is about 1.8 second long.

**[0055]** Other forms of the present technology do not adjust TiMax or Backup Rate, but directly activate triggering and cycling of a ventilator. In one configuration, the ability of the patient for manual intervention may be limited by time constraints.

**[0056]** Figure 4 shows a schematic of a breath on a flow-time curve, provided by a ventilator that is set to be in "Spontaneous" mode (i.e. S mode). Inspiration is shown as positive flow and expiration as shown as negative flow. This figure shows an example breath with a long exhalation portion.

**[0057]** Figure 5 shows a detail from Fig. 4. The Flow axis includes a "trigger flow" threshold TF, and a prior art ventilator may be configured to trigger or provide support to a breath of a patient when measured patient respiratory flow exceeds the "trigger flow" threshold TF. In accordance with the present technology, a supporting breath can be delivered to the patient sooner than would occur in the prior art or in the pre-settings of the ventilator by the patient, e.g., manually, triggering the breath. In Fig. 5, for example, a patient that feels that assistance is needed in order to urge or assist him into inspiration may trigger a supporting breath at an instance indicated by dashed line 20. This may be achieved, as indicated above, by pushing a trigger button. Then, inspiration assistance is provided and inspiration starts. As seen, this will advance the support that a patient may be provided with by a factor of time indicated in this figure as "trigger advance" TAD.

#### 5.1.1.4 Pressure support and EPAP

**[0058]** In another form of the present technology (not

illustrated), the patient manually increases the level of pressure support (e.g. the difference between an IPAP level and an EPAP level) by activation of a button.

**[0059]** In one form of the present technology, not shown, there is a joystick that is used to adjust the level of pressure support. The joystick has a natural neutral position. It may be pushed up, and upon release, it will automatically return to the neutral position. It may also be pushed down, and upon release, it will automatically return to the neutral position.

**[0060]** In one form of the present technology, the apparatus is configured so that once a patient has pushed up and released the joystick, the pressure support will increase by, e.g., 3 cmH2O.

**[0061]** In one form of the present technology, the apparatus is configured so that once a patient has pushed down and released the joystick, the pressure support will decrease by, e.g., 3 cmH2O.

**[0062]** In alternative forms, the amount of change may be different to 3 cmH2O, for example, 1 cmH2O, 2 cmH2O, 4 cmH2O, 5 cmH2O, or some other amount.

**[0063]** Alternatively, moving the joystick may continuously change the provided pressure support. The patient can then decide to lock the instantaneous pressure support achieved at a particular point, or let it automatically return to its initial level. The rate of change of the pressure support, whether driven by the patient or during the automatic return to a predefined rate, may also be predetermined, manually adjustable or both.

**[0064]** For example, in a ventilator delivering a pressure waveform having two levels, namely an inspiratory pressure (IPAP) and an expiratory pressure (PEEP or EPAP), the patient may be able to manually adjust one or both of IPAP and PEEP or EPAP.

**[0065]** In an alternate, regardless of whichever of the IPAP and EPAP are adjusted, the other may also change. The change may be associated with a predetermined function. Thus, in response to the patient's manual control inputs, the IPAP and EPAP will change together, according to this predetermined function relating the change in EPAP with the change in the IPAP.

**[0066]** In one form, the IPAP and EPAP may be approximately related by the function:

$$\Delta (\text{IPAP}) = 3x \Delta (\text{EPAP}),$$

i.e., the patient increasing the IPAP by 3 cmH2O will automatically increase the EPAP by 1 cmH2O.

**[0067]** It has to also be appreciated that in some instances, instead of changing the pressure support, IPAP or EPAP, a patient may manually (or the ventilator automatically) adjust a respective target ventilation level.

**[0068]** Also, whilst any one of a number of ventilation parameters may be individually adjustable by the patient, it is envisaged that similar functionality may be better facilitated by offering various modes of operation of the

ventilator, each mode having specific set of ventilation parameters. For example, instead of being offered a large number of separate parameters for manual adjustment, a patient may be offered three different modes: "resting", "gentle exercise" and "moderate exercise". Each of these modes or states may be associated with a specific set of ventilation parameters, such as respiratory rate, pressure support, target ventilation level, EEP, EPAP etc.

**[0069]** In one form, the patient may manually adjust the pressure waveform provided by the ventilator, by selecting between running values (i.e. non-discrete) or discrete values of metabolic demand appropriate e.g. to the level of activity or work he is experiencing. Selecting a certain metabolic demand accordingly sets a corresponding location along the pathway 21, and together with that a level of EPAP, IPAP and pressure support. Manual selection of the metabolic demand may be performed by e.g. pressing buttons on a remote control.

#### 5.1.1.5 Tidal volume

**[0070]** In one form, the ventilator comprises a control that allows a patient to adjust a tidal volume setting of the ventilator.

#### 5.1.1.6 Oxygen

**[0071]** In one form of the present technology, oxygen is delivered to the patient. In accordance with one form of present technology, a patient may manually increase or decrease the flow rate of oxygen.

#### 5.1.1.7 Humidification

**[0072]** In one form of the present technology, the patient can adjust a level of humidification provided by the ventilator 12 or 4000 by a humidifier 5000 (see e.g. Fig. 9 where device 4000 is shown with humidifier 5000). For example the patient may be able to increase or decrease a level of relative and/or absolute humidity.

#### 5.1.1.8 Temperature

**[0073]** In one form, the patient can adjust a temperature of air delivered.

#### 5.1.1.9 Waveform

**[0074]** In one form of the present technology, the patient can adjust the shape of the pressure waveform. For example, the patient may be able to vary the pressure waveform from a more square wave to a more rounded or smoother waveform. In alternative arrangement, the patient may be able to select a waveform from a set of predefined waveforms.

### 5.1.2 Cruise Control

**[0075]** In another form of the present technology, the apparatus 10 is programmed and configured to operate in a semi-automatic fashion, e.g. to learn a pattern of manually activated triggers, and/or cycles. The ventilator is able to learn from the patient a setting appropriate to the current level of activity. In one form a processor, e.g. 4230, is programmed to execute one or more algorithms as follows. For example, the patient may manually trigger the ventilator 12 or 4000 a number of times over several breaths. The apparatus 10 calculates a patient preferred period between breaths and then upon activation of a "CRUISE CONTROL" mode, delivers breaths at the patient preferred rate.

**[0076]** In one form, the apparatus 10 is programmed and configured to determine a running average duration between manually triggered breaths. In one form the apparatus 10 determines a running average duration between manually cycled breaths.

**[0077]** In one form, the apparatus 10 is programmed and configured to store a time,  $t_0$ , when the manual trigger is first pressed, and also to store the times,  $t_1$ ,  $t_2$ ,  $t_3$  when a new trigger and subsequent triggers are pressed.

For example, the times may be stored in an array of time values  $t(i)$ , having an array index  $i$  by which time values, where  $i$  is an integer, e.g. so that some consecutive time values of  $t(i)$  may be found. The differences  $t_1-t_0$ ,  $t_2-t_1$  and  $t_3-t_2$  are calculated and an average is taken and stored.

**[0078]** In one form, the apparatus 10 is programmed and configured to store a time,  $c_0$ , when a manual cycle is first activated (e.g. by release of a button), and also to store the times,  $c_1$ ,  $c_2$ ,  $c_3$  when subsequent cycles are activated. The differences  $c_1-c_0$ ,  $c_2-c_1$  and  $c_3-c_2$  are calculated and an average is taken and stored.

**[0079]** Figure 6 illustrates three lines: a pressure waveform delivered by a ventilator (top), trigger button signal (middle) and cruise button signal (bottom). When the trigger button is pressed, the ventilator triggers to deliver a breath at a pressure of IPAP, and when it is released, the ventilator cycles to deliver a breath at a pressure of EPAP. The duration of the first inhalation portion of the breathing cycle is  $T_{I1}$ . The duration of the second and third inhalation portions are  $T_{I2}$  and  $T_{I3}$ , respectively. The durations of the first, second and third exhalation portions are  $T_{E1}$ ,  $T_{E2}$  and  $T_{E3}$  respectively.

**[0080]** In one form of the present technology, the apparatus 10 calculates  $T_{Icruise}$ , as the average of the last three inhalations, e.g.  $T_{I1}$ ,  $T_{I2}$  and  $T_{I3}$ ; and furthermore preferably the apparatus 10 calculates  $T_{Ecruise}$ , as the average of the last three exhalations, e.g.  $T_{E1}$ ,  $T_{E2}$  and  $T_{E3}$ . Preferably the average is calculated as a running average, so that if the patient continues to manually trigger and cycle, the average times will be updated. In one form, the average may be calculated from last "k" recent stored time values of  $t(i)$ , with "k" being an integer not exceeding "m", where "m" is a integer between "0" and

"n", the number of samples.

**[0081]** Upon activation of the "CRUISE CONTROL" mode by pressing e.g. the "cruise" button, the ventilator 12 will trigger and subsequently cycle at the average cycle time calculated in the averaging step. See Figure 6, "Cruise Mode On".

**[0082]** For example, as shown in Fig. 6, when Cruise control is activated, the last three inhalations are TI4, TI3 and TI2, and the last three exhalations are TE3, TE2, and TE1.

**[0083]** Hence

$$TI_{cruise} = (TI4 + TI3 + TI2) / 3$$

$$TE_{cruise} = (TE3 + TE2 + TE1) / 3$$

**[0084]** In one form of the present technology, output devices 4290 e.g. feedback lights and/or chimes are included (see Fig. 8b). When the apparatus 10 has sufficient data a light and/or chime at e.g. the ventilator 12 or 4000 will be activated to indicate that the ventilator 12 or 4000 is ready to go into cruise control mode. See Figure 6 "Cruise Ready".

**[0085]** In this way, a patient can adjust a breath length from that which would be delivered but for the patient intervention.

**[0086]** In one form of the present technology, a warning light and/or chime will be activated if the patient attempts to enter cruise control mode when the apparatus 10 is not ready to enter cruise control mode.

**[0087]** In one form of the present technology, an indicator light and/or chime will be activated if the patient successfully enables cruise control mode, and remains activated while cruise control mode is in effect.

### 5.1.3 Response to changing metabolic demand or lung mechanics

**[0088]** Another aspect of one form of the present technology is a device that is constructed and arranged to be able to provide automatically a suitable pressure waveform in response to changing metabolic demand.

**[0089]** Methods and apparatus are provided to determine a suitable pressure waveform, including the steps of adjusting the level of: EPAP, and/or IPAP, and/or pressure support provided to the patient, with pressure support being the difference between EPAP and IPAP.

**[0090]** In another form, providing a sufficient pressure waveform can be performed by following, e.g. at the controller 16, 4230 or ventilator 12, 4000, a predefined continuous support pathway for determining the required pressure waveform for the patient. An example of such a continuous pathway can be seen indicated as 21 in Fig. 7A. Here, the pathway 21 is illustrated by the hatched area and is defined by an EPAP line and an IPAP line,

that respectively bound the pathway from below and above.

**[0091]** According to the pathway 21 of Fig. 7A, as the level of metabolic demand increases, e.g. within a first range of metabolic demand values, the levels of IPAP and EPAP increase together, for example increasing linearly, with it until an inflection point, here indicated by 'dotted line' 17, is reached. As the level of metabolic demand increases beyond this line 17, the level of IPAP also increases, preferably however here at a different rate, optionally lower than before. The EPAP level as seen may be maintained after this point at a constant level, here defined as EPAPmax, which in one form is about 10cmH2O. The level of pressure support in the pathway is accordingly defined for each given value of metabolic demand as the difference between IPAP and EPAP for that given value. Here, the pressure support at a certain value of metabolic demand is indicated by 'double sided arrow' 19.

**[0092]** As seen in Fig. 7B, changes in the level of pressure support may also vary discretely with change in metabolic demand. Here, these discrete changes are obtained by the IPAP and EPAP lines being stepped shaped. The optional lower rate of increase in IPAP level after the inflection point indicated by line 17; is achieved in this pathway by smaller steps of increase in the IPAP level.

**[0093]** In yet another form, pre-defined discrete levels of work or metabolic demand of a patient may be defined, and the apparatus 10 or ventilator 12, 4000 may be configured to enable automatic selection of (or movement between) these discrete levels. Such pre-defined levels may be defined as: (i) Quiet sitting (e.g. when the body is at rest); (ii) Walking around (e.g. when the body is at normal average activity); (iii) Running (e.g. when the body is at a high level of activity). And, the level of e.g. pressure support at each mode can be: (i) Quiet sitting - about 7cmH2O to about 9cmH2O, more preferably about 7cmH2O; at mode (ii) Walking around - about 10cmH2O to about 13cmH2O, more preferably about 11cmH2O; and at mode (iii) Running - about 14cmH2O to about 17cmH2O, more preferably about 15cmH2O.

**[0094]** Optionally, a form of apparatus 10 may be configured to function with such discrete levels of metabolic demand and in addition with the pathway 21. Thus, the dashed lines seen in Fig. 7A indicate the modes (i), (ii) and (iii) of such a form of apparatus 10, and as seen selecting a mode may affect in this form also the level of EPAP and IPAP that is provided to the patient. For example, moving from mode (i) to (ii) may also increase the levels of EPAP and IPAP in addition to pressure support.

### 5.1.4 Rate responsive ventilator

**[0095]** In one form, the pressure waveform provided by the ventilator may be automatically set by detecting changes in metabolic demand e.g. by monitoring one or more of heart rate, breathing (or respiratory) rate, and

movement, or state of movement. In one form of the present technology a sensor configured to provide a measure of metabolic demand, e.g. heart rate and breathing (or respiratory) rates, provides an input to a processor. In one form the metabolic demand responsive sensor is an oximeter 4273 used to detect heart rate and/or respiratory rates (see, e.g., oximeter 4273 indicated in Fig. 8b).

**[0096]** In one form an oximeter 4273 is used to provide a photoplethysmogram (PPG). One or more respiratory parameters are extracted from a PPG signal using a time-domain, and/or a frequency-domain processing step. For example, wavelet-based analysis may be used.

**[0097]** In one form a value for heart rate variability is determined from a signal from an oximeter 4273. The value of heart rate variability is used to estimate a level of activity of the vagal nerve, and to infer a measure of metabolic demand.

**[0098]** In one form, in a further processing step, a respiratory parameter extracted from a PPG signal is used, preferably in conjunction with a parameter extracted from a flow sensor, to estimate a respiratory rate, or as an input to a respiratory rate state machine.

**[0099]** A control algorithm monitors the respiratory rate and in response to a change of respiratory rate, or a change in state of a respiratory rate state machine, adjusts one or more of IPAP and EPAP.

**[0100]** In one example, when the estimated respiratory rate increases, the ventilator or PAP device increases the IPAP level. In a further example, when the estimated respiratory rate increases, the ventilator or PAP device increases the EPAP level.

**[0101]** In one example, when the estimated respiratory rate decreases, the ventilator or PAP device decreases the IPAP level. In a yet further example, when the estimated respiratory rate decreases, the ventilator or PAP device decreases the EPAP level.

**[0102]** In this way the ventilator is able to respond automatically to the respiratory rate of the patient, and to assist the patient to exercise.

**[0103]** In one form, actigraphy, e.g. accelerometers, are used to detect movement of the patient. When a patient starts to walk or exercise, the level of movement of the patient is detected and used to respectively increase at least one of a respiratory rate (e.g. breaths per minute), and/or level of pressure support and/or target ventilation.

**[0104]** In one form, an exercise machine is connected to the ventilator. When a patient begins to exercise, the movement of the machine provides an input to the ventilator to alter a rate and or a level of pressure support or target ventilation.

**[0105]** In one form, a wearable sensor is used to detect movement of the patient and as an input to control the ventilator. For example, a Global Positioning Sensor (GPS) may be used to detect a movement of the patient. The change in location and the corresponding differences in time may indicate the speed of the patient. The measured speed can be used as an indication of whether

and how quickly the patient is moving. Such an indication may then be used to trigger a corresponding change in the ventilation parameters, such as provided respiratory rate, level of pressure support or target ventilation level.

In one configuration, the system may include a lookup table which relates a specific speed with a specific respiratory rate, pressure support or target ventilation level. A maximum speed limit, i.e. higher than 1 m/s, may be imposed and speeds higher than the speed limit may be ignored, as they may be indicative of the patient movement being assisted by a third party or by transportation means.

**[0106]** In one form, an analogue sensor or controller is used that is configured to provide a greater level of support the harder it is pressed. In another form, an analogue sensor or controller is used to trigger and/or cycle the ventilator.

### 5.1.5 Determining EPAP

**[0107]** In one form of the present technology, expiratory pressure level (EPAP) is set automatically to a level at or slightly below the intrinsic positive end expiratory pressure (PEEP), e.g. as determined by reducing or minimising Expiratory Flow Limitation (EFL). The presence of EFL may be determined using a forced oscillation technique.

**[0108]** In one form the presence of EFL is determined using a technique such as that described in Peslin et al. (1993) EUR RESPIR J, 6, 772-784, "Respiratory mechanics studied by forced oscillations during artificial ventilation".

**[0109]** In one form the presence of EFL is determined by applying a sinusoidal pressure waveform, e.g. at 5Hz, 10Hz and 20Hz at the entrance to the airways, e.g. using a loudspeaker placed in parallel with the ventilator, or by applying an oscillatory pressure waveform signal to a blower under the control of a processor. The airway is modelled as a combination of resistance, compliance and in one form, inertance. Complex impedances in inspiration and expiration are determined. Intrinsic PEEP is determined by adjusting EPAP and finding the lowest value of EPAP which reduces the magnitude of the difference between the inspiratory and expiratory values of the imaginary component of complex impedance to a level close to that seen in normal patients, or finding the lowest value of EPAP above which a further increase no longer yields a significant decrease in this difference.

**[0110]** This step of determining an EPAP level using a forced oscillation technique may be combined with a step of determining a respiratory rate from an oximeter 4273 and/or a flow sensor.

### 5.1.6 Patient responsive algorithm

**[0111]** In one form of the present technology, the processor e.g. 4230 is configured to execute an algorithm that includes the following steps:

- (i) Adjust tidal volume and respiratory rate to maintain minute ventilation at a value between a predetermined minimum minute ventilation and a predetermined maximum minute ventilation;
- (ii) Receive a patient initiated synchrony stimulus;
- (iii) Determine a minimum target respiratory rate on the basis of a patient initiated synchrony stimulus; and
- (iv) Adjust respiratory rate in response to the patient initiated synchrony stimulus.

## 5.2 Apparatus/Device

**[0112]** In one form of the present technology, a ventilator 12 takes the form of PAP device 4000.

**[0113]** PAP device 4000 comprises mechanical and pneumatic components 4100, electrical components 4200 and is programmed to execute one or more algorithms 4300. The PAP device preferably has an external housing 4010, preferably formed in two parts, an upper portion 4012 of the external housing 4010, and a lower portion 4014 of the external housing 4010. In alternative forms, the external housing 4010 may include one or more panel(s) 4015. Preferably the PAP device 4000 comprises a chassis 4016 that supports one or more internal components of the PAP device 4000. In one form a pneumatic block 4020 is supported by, or formed as part of the chassis 4016. The PAP device 4000 may include a handle 4018.

**[0114]** The pneumatic path of the PAP device 4000 preferably comprises an inlet air filter 4112, and a pressure device 4140 such as a controllable source of air at positive pressure (preferably a blower 4142). One or more pressure sensors 4152 and flow sensors 4154 are included in the pneumatic path.

**[0115]** The preferred pneumatic block 4020 comprises a portion of the pneumatic path that is located within the external housing 4010.

**[0116]** The PAP device 4000 preferably has an electrical power supply 4210, one or more input devices 4220, a processor 4230, a pressure device controller 4240, one or more protection safety circuits 4250, memory 4260, transducers 4270 and one or more output devices 4290. Electrical components 4200 may be mounted on a single Printed Circuit Board Assembly (PCBA) 4202. In an alternative form, the PAP device 4000 may include more than one PCBA 4202. See, e.g., a component 4200 and a PCBA 4202 indicated in Fig. 8a.

**[0117]** The PAP device 4000 is connected to a patient 1000 via an air circuit 4170 in use, e.g., as indicated in Fig. 9.

## 5.2.1 Electrical components

### 5.2.1.1 Power supply 4210

**[0118]** In one form of the present technology power supply 4210 is internal of the external housing 4010 of the PAP device 4000. In another form of the present technology, power supply 4210 is external of the external housing 4010 of the PAP device 4000.

**[0119]** In one form of the present technology power supply 4210 provides electrical power to the PAP device 4000 only. In another form of the present technology, power supply 4210 provides electrical power to both PAP device 4000 and a humidifier 5000.

**[0120]** In one form of the present technology power supply 4210 is a battery. Preferably the battery has at least enough energy to power the PAP device 4000 to allow a patient to exercise for a period, e.g. about 1 to about 2 hours, alternatively the period is about 2 hours to about 4 hours.

### 5.2.1.2 Input devices 4220

**[0121]** In one form of the present technology, a PAP device 4000 includes one or more input devices 4220 in the form of buttons, switches or dials to allow a person to interact with the device. The buttons, switches or dials may be physical devices, or software devices accessible via a touch screen. The buttons, switches or dials may, in one form, be physically connected to the external housing 4010, or may, in another form, be in wireless communication with a receiver that is in electrical connection to a processor 4230.

**[0122]** In one form the input device 4220 may be constructed and arranged to allow a person to select a value and/or a menu option.

### 5.2.1.3 Processor 4230

**[0123]** In one form of the present technology, a processor 4230 suitable to control a PAP device 4000 is an x86 INTEL processor.

**[0124]** A processor 4230 suitable to control a PAP device 4000 in accordance with another form of the present technology includes a processor based on ARM Cortex-M processor from ARM Holdings. For example, an STM32 series microcontroller from ST MICROELECTRONICS may be used.

**[0125]** Another processor 4230 suitable to control a PAP device 4000 in accordance with a further alternative form of the present technology includes a member selected from the family ARM9-based 32-bit RISC CPUs. For example, an STR9 series microcontroller from ST MICROELECTRONICS may be used.

**[0126]** In certain alternative forms of the present technology, a 16-bit RISC CPU may be used as the processor 4230 for the PAP device 4000. For example a processor from the MSP430 family of microcontrollers, manufac-

tured by TEXAS INSTRUMENTS, may be used.

**[0127]** The processor 4230 is configured to receive input signal(s) from one or more transducers 4270, and one or more input devices 4220.

**[0128]** The processor 4230 is configured to provide output signal(s) to one or more of an output device 4290, and a pressure device controller 4240.

**[0129]** The processor 4230 is configured to implement the one or more algorithms expressed as computer programs stored in memory 4260.

#### 5.2.1.3.1 Clock 4232

**[0130]** Preferably PAP device 4000 includes a clock 4232 that is connected to processor 4230.

#### 5.2.1.4 Pressure device controller 4240

**[0131]** In one form of the present technology, pressure device controller 4240 is located within processor 4230.

**[0132]** In one form of the present technology, pressure device controller 4240 is a dedicated motor control integrated circuit. For example, in one form a MC33035 brushless DC motor controller, manufactured by ONSEMI is used.

#### 5.2.1.5 Protection circuits 4250

**[0133]** Preferably a PAP device 4000 in accordance with the present technology comprises one or more protection circuits 4250.

**[0134]** One form of protection circuit 4250 in accordance with the present technology is an electrical protection circuit.

**[0135]** One form of protection circuit 4250 in accordance with the present technology is a temperature or pressure safety circuit.

#### 5.2.1.6 Memory 4260

**[0136]** In accordance with one form of the present technology the PAP device 4000 includes memory 4260, preferably non-volatile memory. One or more of the algorithms described above are stored in memory 4260 and executed by processor 4230 in use.

**[0137]** In some forms, memory 4260 may include battery powered static RAM. In some forms, memory 4260 may include volatile RAM.

**[0138]** Preferably memory 4260 is located on PCBA 4202. Memory 4260 may be in the form of EEPROM, or NAND flash.

**[0139]** Additionally or alternatively, PAP device 4000 includes removable form of memory 4260, for example a memory card made in accordance with the Secure Digital (SD) standard.

#### 5.2.1.7 Transducers 4270

**[0140]** Transducers may be internal of the device, or external of the PAP device. External transducers may be located for example on or form part of the air delivery circuit, e.g. the patient interface. External transducers may be in the form of non-contact sensors that transmit or transfer data to the PAP device.

##### 5.2.1.7.1 Flow 4271

**[0141]** A flow transducer 4271 in accordance with the present technology may be based on a differential pressure transducer, for example, an SDP600 Series differential pressure transducer from SENSIRION. The differential pressure transducer is in fluid communication with the pneumatic circuit, with one of each of the pressure transducers connected to respective first and second points in a flow restricting element.

**[0142]** In use, a signal from the flow transducer 4271, is received by the processor 4230.

##### 3.2.1.7.2 Pressure 4272

**[0143]** A pressure transducer 4272 in accordance with the present technology is located in fluid communication with the pneumatic circuit. An example of a suitable pressure transducer is a sensor from the HONEYWELL ASDX series. An alternative suitable pressure transducer is a sensor from the NPA Series from GENERAL ELECTRIC.

**[0144]** In use, a signal from the pressure transducer 4272, is received by the processor 4230. In one form, the signal from the pressure transducer 4272 is filtered prior to being received by the processor 4230.

**[0145]** Processor 4230 uses a signal from the pressure transducer 4272 to assist in control of the pressure delivered to the patient 1000 via patient interface 3000.

##### 5.1.1.7.3 Oximeter 4273

**[0146]** An oximeter 4273 in accordance with the present technology may be an oximeter from one of the following manufacturers: PHILIPS, MASIMO, NELLCOR. For example, a NELLCOR OxiMax sensor may be used.

##### 5.2.1.7.4 Electromyograph 4274

**[0147]** In one form of the present technology an electromyograph (EMG) 4274 is provided. The EMG 4274 is configured to monitor activity of the diaphragm of the patient.

##### 5.2.1.8 Output devices 4290

**[0148]** An output device 4290 in accordance with the present technology may take the form of one or more of

a visual, audio and haptic unit. A visual display 4294 may be a Liquid Crystal Display (LCD) or Light Emitting Diode (LED) display, and a display driver 4292 may be used for displaying information on the display 4294.

### 5.3 Additional or alternative aspects

**[0149]** An example form of a device for implementing one or more of the methods of the present technology is illustrated in FIG. 10. In some forms, the apparatus 100 may include a patient respiratory interface 102, a delivery tube 110, a controller 104 and a flow generator such as a servo-controlled blower 105.

**[0150]** The patient respiratory interface such as a mask 108 as shown together with the delivery tube 110, provides a respiratory treatment to the patient's respiratory system via the patient's mouth and/or the patient's nares. Optionally, the patient respiratory interface may be implemented with a nasal mask, nose & mouth mask, full-face mask or nasal pillows or tracheostomy tube.

**[0151]** With the flow generator, the apparatus 100 can be configured to generate a respiratory pressure treatment at the patient respiratory interface. To assist this end, the device may further include a pressure sensor 106, such as a pressure transducer to measure the pressure generated by the blower 105 and generate a pressure signal  $p(t)$  indicative of the measurements of pressure. In such a device, the delivery tube 110 may serve as the sense tube to permit detection of pressure levels supplied to the mask or patient respiratory interface.

**[0152]** The apparatus 100 may also optionally be equipped with a flow sensor 107, which may be coupled with the patient respiratory interface. The flow sensor generates a signal representative of the patient's respiratory flow. The signals from the sensors may be used to detect obstructive or central apneas, hypopneas, cardiogenic airflow, respiratory rates and other respiratory related parameters from the signals measured by the sensors as discussed in more detail herein. In some forms, flow proximate to the mask 108 or delivery tube 110 may be measured using a pneumotachograph and differential pressure transducer or similar device such as one employing a bundle of tubes or ducts to derive a flow signal  $f(t)$ . Alternatively, a pressure sensor may be implemented as a flow sensor and a flow signal may be generated based on the changes in pressure. Although the pressure or flow sensors are illustrated in a housing of the controller 104, they may optionally be located closer to the patient, such as in the mask 108 or delivery tube 110. Other devices for generating a respiratory flow signal or pressure signal may also be implemented. For example, a motor RPM sensor may be utilized to estimate pressure or flow information supplied by the flow generator device based upon the characteristics of the system.

**[0153]** Based on flow  $f(t)$  and/or pressure  $p(t)$  signals, the controller 104 with one or more processors 114 generates blower control signals. For example, the controller may generate a desired pressure set point and servo-

control the blower to meet the set point by comparing the set point with the measured condition of the pressure sensor. Thus, the controller 104 may make controlled changes to the pressure delivered to the patient interface by the blower. Optionally, such changes to pressure may be implemented by controlling an exhaust with a mechanical release valve (not shown) to increase or decrease the exhaust while maintaining a relatively constant blower speed.

**[0154]** With such a controller or processor, the apparatus can be used for many different pressure treatment therapies, such as the pressure treatments for sleep disordered breathing, Cheyne-Stokes Respiration, obstructive sleep apnea (e.g., CPAP, APAP, Bi-Level CPAP, AutoVPAP), etc., or combinations thereof by adjusting a suitable pressure delivery equation. For example, the pressure treatment therapies of the devices described in U.S. Patent Nos. 6,532,957, 6,845,773 and 6,951,217, which are incorporated herein by reference in their entireties, may be implemented with a apparatus 100 of the present technology. For example, as described in these patents, the controller and flow generator may be configured to provide pressure support ventilation. Such a treatment may ensure delivery of a specified or substantially specified target ventilation, for example, a minute ventilation, a gross alveolar ventilation or a alveolar ventilation, to the patient interface during the course of a treatment session by comparing an measure of ventilation with the target ventilation; or delivery of a tidal volume by comparing a measure of tidal volume with a target tidal volume. Thus, if a patient's respiration causes the measured ventilation to fall below or rise above the target ventilation over time, the flow generator will compensate with an increase or decrease respectively in the supplied pressure support ventilation. This may be accomplished with pressure variations that provide a bi-level form of therapy or some other form of therapy that may more smoothly replicate changes in a patient's respiration cycle. While the form of Fig. 10 illustrates a flow generator for generating such pressure support ventilation, as described herein, in some cases a apparatus may be implemented for monitoring without a flow generator for a pressure treatment.

**[0155]** Optionally, the apparatus 100 may also include additional diagnosis sensors 112 that may be contact or non-contact sensors. For example, the device may include an oximeter. The oximeter may generate a signal representative of a blood oxygen level of a patient. A suitable example oximeter or monitor device may optionally be any of the devices disclosed in International Patent Application No. International Application No. PCT/AU2005/001543 (Pub. No. WO/2006/037184) or International Patent Application No. PCT/AU1996/000218 (Pub. No. WO/1996/032055), the disclosures of which are incorporated herein by cross-reference. As disclosed in these incorporated PCT applications, the monitor may serve as diagnosis sensors that can also optionally provide a blood pressure and/or heart or pulse rate monitor

for measuring a heart rate and/or blood pressure of the patient.

**[0156]** In some forms, the diagnosis sensors may also include an ECG monitor. Such a device may be configured to detect cardiac-related characteristics such as a heart rate and may also determine respiratory parameters (such as central or obstructive apneas, hypopneas, etc.) Optionally, these parameters may be determined by the analysis algorithms of controller 104 based on transmission of the ECG data to the controller or they may be determined by the monitor and be transmitted to the controller 104.

**[0157]** In some forms, the diagnosis sensors may include a movement sensor. For example, a suprasternal notch sensor or chest band may be implemented to generate a movement signal that is indicative of patient effort during respiration. Other suitable sensors may include the movement sensing devices disclosed in International Patent Application No. PCT/AU1998/000358 (Pub. No. WO 1998/052467) the disclosure of which is incorporated herein by cross-reference. The movement sensors thus may provide a measure of patient effort and/or respiration rate and may be used as an alternative to a flow sensor or in conjunction with other flow sensors as discussed in more detail herein.

**[0158]** Some forms may monitor respiratory parameters with non-contact infrared or wireless biomotion sensors. One such example is the BiancaMed Doppler device which uses low power pulses of radio frequency energy transmitted and reflected back to a sensor to detect respiration rate, heart rate and movement, etc. Alternatively, or in addition thereto, contact respiratory monitoring devices such as a respiratory band or movement sensitive bed may be implemented to monitor patient respiratory parameters.

**[0159]** The signals from the sensors may be sent to the controller 104. Optional analog-to-digital (A/D) converters/samplers (not shown separately) may be utilized in the event that supplied signals from the sensors are not in digital form and the controller is a digital controller. Based on the signals from the sensor(s), the controller assesses the condition of the patient.

**[0160]** The controller may optionally include a display device 116 such as one or more warning lights (e.g., one or more light emitting diodes). The display device may also be implemented as a display screen such as an LCD or a touch sensitive display. Activation of the display device 116 will typically be set by the controller based on an assessment of the condition by the apparatus 100. The display device may be implemented to visually show information to a user of the apparatus 100 or a clinician or physician. The display device 116 may also show a graphic user interface for operation of the apparatus 100. User, clinician or physician control of the operation of the apparatus 100 may be based on operation of input switches 118 that may be sensed by the controller or processor of the apparatus.

**[0161]** Optionally, the controller may also include a

communications device 120 for receiving and/or transmitting data or messages by the apparatus 100. For example, the communications device may be a wireless transceiver such as Bluetooth or WIFI transceiver. The communications device may also be a network communications device such as a phone modem and/or network card and may be implemented to send messages via the internet directly or through a computer to which the detection device may be docked. The communications device 120 may communicate with a remote device 122.

**[0162]** The controller 104 or processor 114 will typically be configured to implement one or more particular control methodologies such as the algorithms described in more detail herein. Thus, the controller may include integrated chips, a memory and/or other control instruction, data or information storage medium. For example, programmed instructions encompassing such a control methodology may be coded on integrated chips in the memory of the device. Such instructions may also or alternatively be loaded as software or firmware using an appropriate data storage medium. In still further forms, control over parameters of treatment may be set in accordance with a patient synchronization demand so as to permit a suitable treatment for mobility or exercise.

**[0163]** Some forms of the present technology involve an apparatus to generate pressure support ventilation. The apparatus may include at least one sensor adapted to measure at least one respiratory parameter and a flow generator adapted for coupling with a patient respiratory interface. The flow generator may be configured to provide a flow of breathable gas for pressure support ventilation to the patient respiratory interface. The apparatus may also include a controller coupled to the at least one sensor and the flow generator. The controller may be configured to control the pressure support ventilation with the flow generator. The controller may also be further configured with a rest mode and an exercise mode, the rest mode having a first value set of control parameters for the pressure support ventilation and the exercise mode having a second value set of control parameters for the pressure support ventilation.

**[0164]** In some cases, the controller may be configured to receive a user activated trigger stimulus, and, in response to the trigger stimulus to select the second value set of control parameters for the exercise mode. In response to the trigger stimulus, the controller may set a target respiratory control parameter as a function of a presently detected respiratory parameter sensed with the sensor. The target respiratory control parameter may be a target respiratory rate and the detected respiratory parameter may be a measured respiratory rate. The target respiratory control parameter may be a target ventilation and the detected respiratory parameter may be a measure of ventilation. Optionally, the target ventilation may be a target tidal volume and the measure of ventilation may be a measure of tidal volume. Still further, the target ventilation may be a target minute ventilation and the measure of ventilation may be a measure of minute ven-

tilation. In some cases, the second value set of control parameters may comprise an increase in target values with respect to the first value set of control parameters.

**[0165]** Optionally, the apparatus may further include at least one user accessible button to activate the controller such that the button may be configured for actuating the trigger stimulus. Still further, the apparatus may also include a diaphragm electromyogram sensor to activate the controller such that the sensor may be configured for actuating the trigger stimulus. In some cases, the apparatus may include a vagal nerve sensor to activate the controller such that the sensor may be configured for actuating the trigger stimulus.

**[0166]** In some cases, the controller of the apparatus may be further configured with a cool down mode, and configured to receive another user activated trigger stimulus to initiate the cool down mode. The cool down mode may include a third value set of control parameters for the pressure support ventilation. The controller may be configured such that a value of the control parameters of the cool down mode may be varied from a respective value of the control parameters of the exercise mode toward a respective value of the control parameters of the rest mode. The controller may be configured such that a value of the control parameters of the cool down mode may be ramped from a respective value of the control parameters of the exercise mode toward a respective value of the control parameters of the rest mode.

**[0167]** Some forms of the present technology may involve a method for control of pressure support ventilation. The method may include measuring at least one respiratory parameter with a sensor. It may also include generating pressure support ventilation with a flow generator adapted for coupling with a patient respiratory interface. It may further include controlling, with a processor, the pressure support ventilation in a rest mode and an exercise mode. The rest mode may have a first value set of control parameters for controlling the pressure support ventilation and the exercise mode may have a second value set of control parameters for controlling the pressure support ventilation.

**[0168]** The method may further include receiving a user activated trigger stimulus, and, in response to the trigger stimulus, selecting the second value set of control parameters for the exercise mode. The method may also include, in response to the trigger stimulus, setting a target respiratory control parameter as a function of a presently detected respiratory parameter sensed with the sensor. The target respiratory control parameter may be a target respiratory rate and the detected respiratory parameter may be a measured respiratory rate. The target respiratory control parameter may be a target ventilation and the detected respiratory parameter may be a measure of ventilation. The target ventilation may be a target tidal volume and the measure of ventilation may be a measure of tidal volume. The target ventilation may be a target minute ventilation and the measure of ventilation may be a measure of minute ventilation. The second set

of control parameters may include an increase in target values with respect to the first value set of control parameters. In some such methods, a user accessible button actuates the trigger stimulus. In some such methods, a diaphragm electromyogram sensor actuates the trigger stimulus. Still further, in some such methods, a vagal nerve sensor actuates the trigger stimulus.

**[0169]** Optionally, the methods may also include controlling pressure support ventilation in a cool down mode in response to receiving another user activated trigger stimulus, the cool down mode may have a third value set of control parameters for the pressure support ventilation. In some cases, a value of the control parameters of the cool down mode may be varied from a respective value of the control parameters of the exercise mode toward a respective value of the control parameters of the rest mode. In some cases, a value of the control parameters of the cool down mode may be ramped from a respective value of the control parameters of the exercise mode toward a respective value of the control parameters of the rest mode.

**[0170]** In some forms, the apparatus 100, such as when implemented to provide a pressure treatment to patient suffering respiratory insufficiency, COPD or other similar ailments, may serve to enhance physical activity or mobility for a patient. For example, the apparatus may be implemented to provide non-invasive ventilation to provide respiratory support for patients during mobility. Such a non-invasive ventilation may enhance exercise capacity in COPD patients or emphysemic patients. Thus, in some forms, a pressure treatment methodology, such as a control algorithm for non-invasive pressure support ventilation, may be implemented to promote exercise or patient mobility with suitable pressure support modes.

**[0171]** As a COPD patient gradually exercises, their tidal volume and respiratory rate will increase. When the patient then rests, the tidal volume and respiratory rate decreases. In some forms of the present technology, a patient-responsive non-invasive ventilation methodology of the apparatus may be configured to adapt to patients' varying respiratory needs during exertion or exercise.

**[0172]** Accordingly, FIG. 11 illustrates an example of a methodology of a controller for such an apparatus. During use, the controller will generally permit a change to pressure support control parameters, such as an increase in ventilation (e.g., tidal volume) and respiratory rate at levels, that are suitable for exercise or mobility up to a maximum ventilation, such as a minute ventilation, and/or maximum respiratory rate so as to provide pressure support at those levels. In order to achieve the desired levels, the apparatus may be configured to respond to a user or patient stimulus for setting the synchronization of the apparatus with the patient's exercise requirements.

**[0173]** For example, the apparatus may provide NIV at initial levels in a rest mode to provide a pressure support suitable for a patient at rest at 400. Thus, the apparatus may begin treatment by accessing stored values

of target parameters for the rest mode where those values of the target parameters are suitable for controlling ventilation or pressure support for patient rest. The user or patient may then begin to exercise. During exercise or shortly before, the patient may then provide a stimulus, such as executing a trigger, to initiate a modification procedure of the apparatus so that the apparatus may begin an exercise mode at 401. The modification procedure permits the values of the target parameters of the pressure support to be modified or set such that the pressure support will be provided at more suitable levels (e.g., increases in target ventilation (e.g., minute ventilation or tidal volume) or in target respiratory rate, or in the maximum or minimum values suitable for controlling pressure support) for exercise at 402. Thus, the modification procedure of the exercise mode may allow enforcement of different minimum and/or maximum values and/or target values of respiratory control parameters in the exercise mode at 403 from the rest mode.

**[0174]** In some such forms, the triggered change or increase to the values of the control parameters of the pressure support ventilation for the exercise mode may optionally be predetermined. In such a case, the executed trigger may result in the apparatus accessing one or more stored values for the control parameters for the pressure support where the stored values of the control parameters are associated with the exercise mode. Such target, minimum and/or maximum values may be previously entered by a physician or clinician. For example, a respiratory rate target or ventilation target may be set as a physician selectable proportional function of the values of the control parameters of the rest mode so as to permit a proportional increase (or decrease) of the parameters from the rest mode. Optionally, in some forms, some of the values of the control parameters of the pressure support ventilation of the exercise mode may be learned so as to better synchronize with the level exercise of the user or patient. For example, the apparatus may learn the exercise respiratory rate, minute ventilation and/or tidal volume of the patient during an initial exercise period of the exercise mode or in response to a stimulus signal of the patient, such as by measuring these parameters from a flow signal in the initial period. Thereafter, such learned values may then be set for the control parameters of a later time period of the exercise mode.

**[0175]** In some forms, the stimulus for entering the exercise mode or making an adjustment to target values to accommodate the patient's state of exercise may be made by the patient by pressing a button of the treatment apparatus or a button on a remote control (e.g., a wired, wireless or infrared transmitter to transmit to an exercise mode signal or exercise synchronization signal to a receiver of the apparatus). Alternatively, the stimulus signal may be a detected physiological stimulus such as for example, a signal from a diaphragm electromyogram sensor, a signal from a sensor that is responsive to activation of the vagal nerve e.g. an oximeter, or an evaluation of a signal from a flow sensor.

**[0176]** In some forms, as further illustrated in FIG. 11, the apparatus may be configured to receive additional stimulus signals or executed triggers from the patient as the exercise progresses or cools down in or from the exercise mode. For example, with each additional stimulus signal, a new set of control values may be established. For example, at 404 a patient or user may trigger learning or loading of a further set of values for the control parameters. The new targets may then be set as the control parameters for the delivery of the pressure support ventilation at 405. The apparatus 100 may then control the pressure support in accordance with the new settings at 403. Each set of control values may be higher or lower than the previous control values based on an increase or decrease of activity.

**[0177]** For example, in some forms, the exercise mode may have a predetermined time interval, such as a maximum time set by a physician or clinician. In some such forms, a timer may begin when the exercise mode starts and the mode may terminate when a preset maximum time is reached. During the exercise mode, the apparatus may deliver pressure support ventilation with the exercise mode control values that are suitable for patient exercise. At the conclusion of the exercise mode, the apparatus may switch to the rest mode, so as to deliver pressure support ventilation with the rest mode control values that are suitable for patient rest. Optionally, the apparatus or remote control may include a button to terminate the exercise mode before the maximum time is reached.

**[0178]** Still further, in some forms, the termination of the exercise mode may initiate a cool down mode. During the cool down mode, the values of the control parameters may be varied over a selectable period of time. For example, the values may be ramped from the values of the target parameters of the exercise mode to the values of the target parameters of the rest mode. For example, the respiratory rate and/or ventilation targets may be automatically modified so as to ramp down or be gradually stepped down over a period of time to the rest mode values.

#### 5.4 Other aspects

**[0179]** The present technology may be packaged as an exercise module or accessory to be used with a range of different ventilators.

**[0180]** Preferably the parameters that are adjustable by the patient are adjustable within limits. Such limits may be established by a clinician prior to use by the patient.

#### 5.5 Advantages

**[0181]** One advantage of the present technology is that it allows ventilators to more closely match a patient's need, particularly in the face of a changing need, e.g. increasing or decreasing, such as when a patient attempts to exercise.

**[0182]** An advantage of the present technology is that

it is easier and more comfortable for patients to use when compared to a ventilator that may have one fixed setting of e.g. minute ventilation, or pressure support.

**[0183]** In addition, the present technology allows a patient to pre-empt a need for a sooner breath, or an increased level of support. By pressing on the relevant button momentarily before they require a breath, the system can respond just as the patient actually needs the breath.

**5.6 Reference signs list**

apparatus	10
ventilator	12
button	14
pc	16
digital communication interface	18
inflection point	17
pressure support	19
Pathway	21
Apparatus	100
Patient respiratory interface	102
Controller	104
Blower	105
Pressure sensor	106
Flow sensor	107
Mask	108
Delivery tube	110
Additional diagnosis sensors	112
Processor	114
Display device	116
Input switches	118
Communications device	120
Remote device	122
Patient interface	3000
pap device	4000
external housing	4010
panel	4015
chassis	4016
handle	4018
pneumatic block	4020
pneumatic component	4100
inlet air filter	4112
blower	4142
pressure sensor	4152
flow sensor	4154
Air circuit	4170
electrical component	4200
PCBA	4202
power supply	4210
input device	4220
processor	4230
clock	4232
pressure device controller	4240
protection circuit	4250

(continued)

memory	4260
transducer	4270
flow transducer	4271
pressure transducer	4272
Oximeter	4273
Electromyograph	4274
output device	4290
algorithm	4300
humidifier	5000

**5.7 Other remarks**

**[0184]** Unless the context clearly dictates otherwise and where a range of values is provided, it is understood that each intervening value, to the tenth of the unit of the lower limit, between the upper and lower limit of that range, and any other stated or intervening value in that stated range is encompassed within the technology. The upper and lower limits of these intervening ranges, which may be independently included in the intervening ranges, are also encompassed within the technology, subject to any specifically excluded limit in the stated range. Where the stated range includes one or both of the limits, ranges excluding either or both of those included limits are also included in the technology.

**[0185]** Furthermore, where a value or values are stated herein as being implemented as part of the technology, it is understood that such values may be approximated, unless otherwise stated, and such values may be utilized to any suitable significant digit to the extent that a practical technical implementation may permit or require it.

**[0186]** Unless defined otherwise, all technical and scientific terms used herein have the same meaning as commonly understood by one of ordinary skill in the art to which this technology belongs. Although any methods and materials similar or equivalent to those described herein can also be used in the practice or testing of the present technology, a limited number of the exemplary methods and materials are described herein.

**[0187]** When a particular material is identified as being preferably used to construct a component, obvious alternative materials with similar properties may be used as a substitute.

**[0188]** It must be noted that as used herein and in the appended claims, the singular forms "a", "an", and "the" include their plural equivalents, unless the context clearly dictates otherwise.

**[0189]** All publications mentioned herein are incorporated by reference to disclose and describe the methods and/or materials which are the subject of those publications. The publications discussed herein are provided solely for their disclosure prior to the filing date of the present application. Nothing herein is to be construed as an admission that the present technology is not entitled to antedate such publication by virtue of prior invention.

Further, the dates of publication provided may be different from the actual publication dates, which may need to be independently confirmed.

**[0190]** Moreover, in interpreting the disclosure, all terms should be interpreted in the broadest reasonable manner consistent with the context. In particular, the terms "comprises" and "comprising" should be interpreted as referring to elements, components, or steps in a non-exclusive manner, indicating that the referenced elements, components, or steps may be present, or utilized, or combined with other elements, components, or steps that are not expressly referenced.

**[0191]** The subject headings used in the detailed description are included only for the ease of reference of the reader and should not be used to limit the subject matter found throughout the disclosure or the claims. The subject headings should not be used in construing the scope of the claims or the claim limitations.

**[0192]** Although the technology herein has been described with reference to particular embodiments, it is to be understood that these embodiments are merely illustrative of the principles and applications of the technology. In some instances, the terminology and symbols may imply specific details that are not required to practice the technology. For example, although the terms "first" and "second" may be used, unless otherwise specified, they are not intended to indicate any order but may be utilised to distinguish between distinct elements. Furthermore, although process steps in the methodologies may be described or illustrated in an order, such an ordering is not required. Those skilled in the art will recognize that such ordering may be modified and/or aspects thereof may be conducted concurrently or even synchronously.

**[0193]** It is therefore to be understood that numerous modifications may be made to the illustrative embodiments and that other arrangements may be devised without departing from the spirit and scope of the technology.

**[0194]** The following aspects are preferred embodiments of the invention:

- 1. A controller for a ventilator, the ventilator being configured to deliver a pressure support waveform to a patient, said pressure support waveform having an inspiratory phase and a subsequent expiratory phase, and the controller being configured to adjust at least one parameter of the ventilator in response to indication of a change in metabolic demand and/or lung mechanics of the patient.
- 2. The controller of aspect 1, wherein the controller is further configured to accept a signal from a metabolic demand responsive transducer, and to determine a state of metabolic demand from said metabolic demand responsive transducer.
- 3. The controller of aspect 2, wherein said metabolic demand responsive transducer is an oximeter.

5

10

15

20

25

30

35

40

45

50

55

4. The controller of aspect 2, wherein said metabolic demand responsive transducer is a flow sensor.

5. The controller of aspect 2, wherein said metabolic demand responsive transducer is a diaphragm electromyograph.

6. The controller of aspect 2, wherein said metabolic demand responsive transducer is a combination of a flow sensor and an electromyograph.

7. The controller of anyone of aspects 1 - 6, wherein the at least one parameter of the ventilator comprises one or more of: an inspiratory pressure during the inspiratory phase, an expiratory pressure during the expiratory phase, and a level of pressure support.

8. The controller of aspect 7, wherein when the at least one parameter of the ventilator comprises the inspiratory pressure, the controller is configured so that a first increase in a level of metabolic demand results in a second increase in a level of the inspiratory pressure.

9. The controller of aspects 7 or 8, wherein when the at least one parameter of the ventilator comprises the pressure support, the controller is configured so that the first increase in a level of metabolic demand results in a third increase in a level of pressure support.

10. The controller of any one of aspects 7 to 9, wherein when the at least one parameter of the ventilator comprises the expiratory pressure, and at least up to a predetermined limit of metabolic demand, the controller is configured so that the first increase in a level of metabolic demand results in a fourth increase in a level of the expiratory pressure.

11. The controller of aspect 10, wherein after the predetermined limit, the controller is configured so that a level of expiratory positive air pressure will remain substantially constant for an additional increase in level of metabolic demand.

12. The controller of any one of aspects 1 to 11, wherein at least for a range of metabolic demand values, the controller is configured to linearly adjust the at least one parameter of the ventilator in response to a change in metabolic demand values in the range.

13. The controller of any one of aspects 1 to 11, wherein at least for a range of metabolic demand values, the controller is configured to discretely adjust between metabolic demand values in the range.

14. The controller of any one of aspects 1 to 13,

wherein an indication of change in metabolic demand and/or lung mechanics is input manually.

15. The controller of any one of aspects 1 to 14, wherein an indication of change in metabolic demand and/or lung mechanics is determined automatically. 5

16. A controller for a ventilator, the ventilator configured to deliver a pressure support waveform, said pressure support waveform comprising an inspiratory phase and a subsequent expiratory phase, and the controller being configured to allow a patient to manually adjust the pressure support waveform. 10

17. The controller of aspect 16, wherein the manual adjustment comprises triggering a breath, preferably by temporarily lowering a minimum number of breaths that the ventilator is configured to deliver per minute. 15

18. The controller of aspect 17, configured so that a manual triggering of a breath is only possible during an EPAP phase. 20

19. The controller of aspect 18, configured so that a manual triggering of a breath is only possible during a defined portion of the EPAP phase. 25

20. The controller of any one of aspects 17, 18 or 19 and being associated with a control member for the manual adjustment of the waveform, and triggering is performed by pressing the control member. 30

21. The controller of any one of aspects 17, 18, 19 or 20 and being configured to store an array of time values  $t(i)$  when each trigger is activated, with "i" being an array index assigned to identify each new trigger, and wherein the controller is further configured to allow a patient to manually adjust a breath length of the waveform according to at least some of the time values of  $t(i)$ . 35

22. The controller of aspect 21, wherein the manual adjustment of the breath length comprises computing differences between at least some consecutive time values of  $t(i)$ . 40

23. The controller of aspect 22, wherein the manual adjustment of the breath length additionally comprises computing an average of at least some of these differences. 45

24. The controller of any one of aspects 21 to 23, wherein "i" is equal to "0" for a first occurring trigger and to "n" for a last recent occurring trigger, and the controller is configured to allow manual adjustment of the breath length only when "i" > "m", with "m" 50

being an integer between "0" and "n".

25. The controller of aspect 24, wherein the at least some of the time values of  $t(i)$  are the last "k" recent stored time values of  $t(i)$ , with "k" being an integer not exceeding "m".

26. The controller of aspect 25, wherein "k" is equal to "m".

27. The controller of any one of aspects 24-26, wherein "m" is equal to 3.

28. The controller of aspect 16, wherein the manual adjustment comprises cycling a breath, preferably by temporarily lowering a maximum time that the ventilator is configured to wait from commencement of an inspiratory phase before automatically changing into an EPAP phase. 20

29. The controller of aspect 28, configured so that manual cycling of a breath is only possible during an inspiratory phase.

30. The controller of aspect 29, configured so that manual cycling is only possible during a defined portion of the inspiratory phase. 25

31. The controller of any one of aspects 28, 29 or 30 and being associated with a control member for the manual adjustment of the waveform, and cycling is performed by releasing the control member. 30

32. The controller of any one of aspects 28, 29, 30 or 31 and being configured to store an array of time values  $t(i)$  when each breath is cycled, with "i" being an array index assigned to identify each time value when a breath is cycled, and wherein the controller is further configured to allow a patient to manually adjust a breathing cycle of the waveform according to at least some of the time values of  $t(i)$ . 35

33. The controller of aspect 32, wherein the manual adjustment of the breathing cycle comprises computing differences between at least some consecutive time values of  $t(i)$ . 40

34. The controller of aspect 33, wherein the manual adjustment of the breathing cycle additionally comprises computing an average of at least some of these differences. 45

35. The controller of any one of aspects 32-34, wherein "i" is equal to "0" for a first occurring cycle and to "n" for a last recent occurring cycle, and the controller is configured to allow manual adjustment of the breathing cycle only when "i" > "m", with "m" being an integer between "0" and "n". 50

36. The controller of aspect 35, wherein the at least some of the time values of  $t(i)$  are the last "k" recent stored time values of  $t(i)$ , with "k" being an integer not exceeding "m". 5
37. The controller of aspect 36, wherein "k" is equal to "m".
38. The controller of any one of aspects 35-37, wherein "m" is equal to 3. 10
39. The controller of aspect 16 and being associated with a control member for the manual adjustment of the waveform and activating the control member increases a level of pressure during the inspiratory phase. 15
40. The controller of aspect 39, wherein the controller is configured so that increasing the level of pressure during an inspiratory phase automatically affects a level of pressure during an expiratory phase. 20
41. The controller of aspect 40, wherein the controller is configured so that the level of pressure during the inspiratory phase is linearly related to the level of pressure during the expiratory phase. 25
42. The controller of aspect 41, programmed so that a magnitude of change to the pressure during the expiratory phase is equal to about one third of a magnitude of change during the inspiratory phase. 30
43. A controller for a ventilator, the ventilator being configured to deliver a pressure support waveform consisting of an inspiratory phase and a subsequent expiratory phase, and the controller being configured to receive one or more signals indicative of a state of a patient and in response to the one or more signals indicative of a state of the patient automatically adjust the pressure support waveform. 35 40
44. The controller of aspect 43, wherein the signals are indicative of a state of movement of the patient. 45
45. The controller of aspect 44, wherein the signals indicate a speed of movement of the patient.
46. The controller of aspect 43, wherein signals are indicative of a heart rate or a respiratory rate of the patient. 50
47. The controller of any one of aspects 43-41, wherein automatically adjusting the pressure support waveform comprises adjusting at least one of the following: a pressure support, a target ventilation level, IPAP, EPAP, a minimum number of breaths that the ventilator is configured to deliver per minute, and a maximum time that the ventilator is configured to wait from commencement of an inspiratory phase before automatically changing into a subsequent expiratory phase. 55
48. A ventilator for providing ventilatory support to a patient, the ventilator comprising:
- a power supply;
  - a controller as claimed in any of the previous aspects; and
  - a pressure device under the control of the controller.
49. Apparatus for providing ventilatory assistance to a patient to assist in exercising comprising a ventilator as claimed in aspect 48, and a metabolic demand responsive transducer.
50. A method of automatically setting an expiratory pressure level in a ventilator to overcome intrinsic positive end expiratory pressure comprising the steps of:
- applying an oscillatory pressure waveform to a patient's airway;
  - determining a complex impedance of the patient's airway during inhalation and exhalation; and
  - Setting an expiratory pressure level at a lowest value of expiratory pressure that reduces a magnitude of a difference between an inspiratory and an expiratory value of an imaginary component of complex impedance to a level close to that seen in normal patients, or finding the lowest value of expiratory pressure above which a further increase no longer yields a significant decrease in this difference.
51. An apparatus to generate pressure support ventilation, comprising:
- at least one sensor adapted to measure at least one respiratory parameter;
  - a flow generator adapted for coupling with a patient respiratory interface, the flow generator configured to provide a flow of breathable gas for pressure support ventilation to the patient respiratory interface; and
  - a controller, coupled to the at least one sensor and the flow generator, the controller configured

to control the pressure support ventilation with the flow generator, the controller being further configured with a rest mode and an exercise mode, the rest mode comprising a first value set of control parameters for the pressure support ventilation and the exercise mode comprising a second value set of control parameters for the pressure support ventilation.

52. The apparatus of aspect 51 wherein the controller is configured to receive a user activated trigger stimulus, and, in response to the trigger stimulus to select the second value set of control parameters for the exercise mode.

53. The apparatus of aspect 52 wherein, in response to the trigger stimulus, the controller sets a target respiratory control parameter as a function of a presently detected respiratory parameter sensed with the sensor.

54. The apparatus of aspect 53 wherein the target respiratory control parameter is a target respiratory rate and the detected respiratory parameter is a measured respiratory rate.

55. The apparatus of aspect 53 wherein the target respiratory control parameter is a target ventilation and the detected respiratory parameter is a measure of ventilation.

56. The apparatus of aspect 55 wherein the target ventilation is a target tidal volume and the measure of ventilation is a measure of tidal volume.

57. The apparatus of aspect 55 wherein the target ventilation is a target minute ventilation and the measure of ventilation is a measure of minute ventilation.

58. The apparatus of aspect 55 wherein the second value set of control parameters comprises an increase in target values with respect to the first value set of control parameters.

59. The apparatus of aspect 52 further comprising at least one user accessible button to activate the controller, the button being configured for actuating the trigger stimulus.

60. The apparatus of aspect 52, further comprising a diaphragm electromyogram sensor to activate the controller, the sensor being configured for actuating the trigger stimulus.

61. The apparatus of aspect 52, further comprising a vagal nerve sensor to activate the controller, the sensor being configured for actuating the trigger

stimulus.

62. The apparatus of aspect 51, wherein the controller is further configured with a cool down mode, and to receive another user activated trigger stimulus to initiate the cool down mode, the cool down mode comprising a third value set of control parameters for the pressure support ventilation.

63. The apparatus of aspect 52 wherein a value of the control parameters of the cool down mode is varied from a respective value of the control parameters of the exercise mode toward a respective value of the control parameters of the rest mode.

64. The apparatus of aspect 63 wherein a value of the control parameters of the cool down mode is ramped from a respective value of the control parameters of the exercise mode toward a respective value of the control parameters of the rest mode.

65. A method for control of pressure support ventilation, comprising:

measuring at least one respiratory parameter with a sensor;

generating pressure support ventilation with a flow generator adapted for coupling with a patient respiratory interface; and

controlling, with a processor, the pressure support ventilation in a rest mode and an exercise mode, the rest mode comprising a first value set of control parameters for controlling the pressure support ventilation and the exercise mode comprising a second value set of control parameters for controlling the pressure support ventilation.

66. The method of aspect 65 further comprising receiving a user activated trigger stimulus, and, in response to the trigger stimulus, selecting the second value set of control parameters for the exercise mode.

67. The method of aspect 66 further comprising, in response to the trigger stimulus, setting a target respiratory control parameter as a function of a presently detected respiratory parameter sensed with the sensor.

68. The method of aspect 67 wherein the target respiratory control parameter is a target respiratory rate and the detected respiratory parameter is a measured respiratory rate.

69. The method of aspect 67 wherein the target res-

piratory control parameter is a target ventilation and the detected respiratory parameter is a measure of ventilation.

70. The method of aspect 69 wherein the target ventilation is a target tidal volume and the measure of ventilation is a measure of tidal volume. 5

71. The method of aspect 69 wherein the target ventilation is a target minute ventilation and the measure of ventilation is a measure of minute ventilation. 10

72. The method of aspect 69 wherein the second set of control parameters comprises an increase in target values with respect to the first value set of control parameters. 15

73. The method of aspect 66, wherein a user accessible button actuates the trigger stimulus. 20

74. The method of aspect 66, wherein a diaphragm electromyogram sensor actuates the trigger stimulus.

75. The method of aspect 66, wherein a vagal nerve sensor actuates the trigger stimulus. 25

76. The method of aspect 66, further comprising controlling pressure support ventilation in a cool down mode in response to receiving another user activated trigger stimulus, the cool down mode comprising a third value set of control parameters for the pressure support ventilation. 30

77. The method of aspect 76 wherein a value of the control parameters of the cool down mode is varied from a respective value of the control parameters of the exercise mode toward a respective value of the control parameters of the rest mode. 35

78. The method of aspect 76 wherein a value of the control parameters of the cool down mode is ramped from a respective value of the control parameters of the exercise mode toward a respective value of the control parameters of the rest mode. 40

## Claims

1. An apparatus to generate pressure support ventilation, comprising: 50

at least one sensor adapted to measure at least one respiratory parameter;  
a flow generator adapted for coupling with a patient respiratory interface, the flow generator configured to provide a flow of breathable gas for pressure support ventilation to the patient 55

respiratory interface; and  
a controller, coupled to the at least one sensor and the flow generator, the controller configured to control the pressure support ventilation with the flow generator, the controller being further configured with a rest mode and an exercise mode, the rest mode comprising a first value set of control parameters for the pressure support ventilation and the exercise mode comprising a second value set of control parameters for the pressure support ventilation.

2. The apparatus of claim 1 wherein the controller is configured to receive a user activated trigger stimulus, and, in response to the trigger stimulus to select the second value set of control parameters for the exercise mode.

3. The apparatus of claim 2 wherein, in response to the trigger stimulus, the controller sets a target respiratory control parameter as a function of a presently detected respiratory parameter sensed with the sensor.

4. The apparatus of claim 3 wherein the target respiratory control parameter is a target respiratory rate and the detected respiratory parameter is a measured respiratory rate.

5. The apparatus of claim 3 wherein the target respiratory control parameter is a target ventilation and the detected respiratory parameter is a measure of ventilation.

6. The apparatus of claim 5 wherein the target ventilation is a target tidal volume and the measure of ventilation is a measure of tidal volume.

7. The apparatus of claim 5 wherein the target ventilation is a target minute ventilation and the measure of ventilation is a measure of minute ventilation. 40

8. The apparatus of claim 5 wherein the second value set of control parameters comprises an increase in target values with respect to the first value set of control parameters. 45

9. The apparatus of any one of claims 2 to 8 further comprising at least one user accessible button to activate the controller, the button being configured for actuating the trigger stimulus.

10. The apparatus of any one of claims 2 to 8, further comprising a diaphragm electromyogram sensor to activate the controller, the sensor being configured for actuating the trigger stimulus.

11. The apparatus of any one of claims 2 to 10, further

- comprising a vagal nerve sensor to activate the controller, the sensor being configured for actuating the trigger stimulus.
- 12.** The apparatus of any one of the previous claims, wherein the controller is further configured with a cool down mode, and to receive another user activated trigger stimulus to initiate the cool down mode, the cool down mode comprising a third value set of control parameters for the pressure support ventilation.
- 13.** The apparatus of claim 12 wherein a value of the control parameters of the cool down mode is varied from a respective value of the control parameters of the exercise mode toward a respective value of the control parameters of the rest mode.
- 14.** The apparatus of claim 13 wherein a value of the control parameters of the cool down mode is ramped from a respective value of the control parameters of the exercise mode toward a respective value of the control parameters of the rest mode.
- 15.** A method for control of pressure support ventilation, comprising:
- measuring at least one respiratory parameter with a sensor; generating pressure support ventilation with a flow generator adapted for coupling with a patient respiratory interface; and controlling, with a processor, the pressure support ventilation in a rest mode and an exercise mode, the rest mode comprising a first value set of control parameters for controlling the pressure support ventilation and the exercise mode comprising a second value set of control parameters for controlling the pressure support ventilation.
- 16.** The method of claim 15 further comprising receiving a user activated trigger stimulus, and, in response to the trigger stimulus, selecting the second value set of control parameters for the exercise mode.
- 17.** The method of claim 16 further comprising, in response to the trigger stimulus, setting a target respiratory control parameter as a function of a presently detected respiratory parameter sensed with the sensor.
- 18.** The method of claim 17 wherein the target respiratory control parameter is a target respiratory rate and the detected respiratory parameter is a measured respiratory rate.
- 19.** The method of claim 17 wherein the target respiratory control parameter is a target ventilation and the detected respiratory parameter is a measure of ventilation.
- 20.** The method of claim 19 wherein the target ventilation is a target tidal volume and the measure of ventilation is a measure of tidal volume.
- 21.** The method of claim 19 wherein the target ventilation is a target minute ventilation and the measure of ventilation is a measure of minute ventilation.
- 22.** The method of claim 19 wherein the second set of control parameters comprises an increase in target values with respect to the first value set of control parameters.
- 23.** The method of any one of claims 16 to 22, wherein a user accessible button actuates the trigger stimulus.
- 24.** The method of any one of claims 16 to 23, wherein a diaphragm electromyogram sensor actuates the trigger stimulus.
- 25.** The method of any one of claims 16 to 24, wherein a vagal nerve sensor actuates the trigger stimulus.
- 26.** The method of any one of claims 16 to 25, further comprising controlling pressure support ventilation in a cool down mode in response to receiving another user activated trigger stimulus, the cool down mode comprising a third value set of control parameters for the pressure support ventilation.
- 27.** The method of claim 26 wherein a value of the control parameters of the cool down mode is varied from a respective value of the control parameters of the exercise mode toward a respective value of the control parameters of the rest mode.
- 28.** The method of claim 27 wherein a value of the control parameters of the cool down mode is ramped from a respective value of the control parameters of the exercise mode toward a respective value of the control parameters of the rest mode.
- 29.** A controller for a ventilator, the ventilator being configured to deliver a pressure support waveform to a patient, said pressure support waveform having an inspiratory phase and a subsequent expiratory phase, and the controller being configured to adjust at least one parameter of the ventilator in response to indication of a change in metabolic demand and/or lung mechanics of the patient.

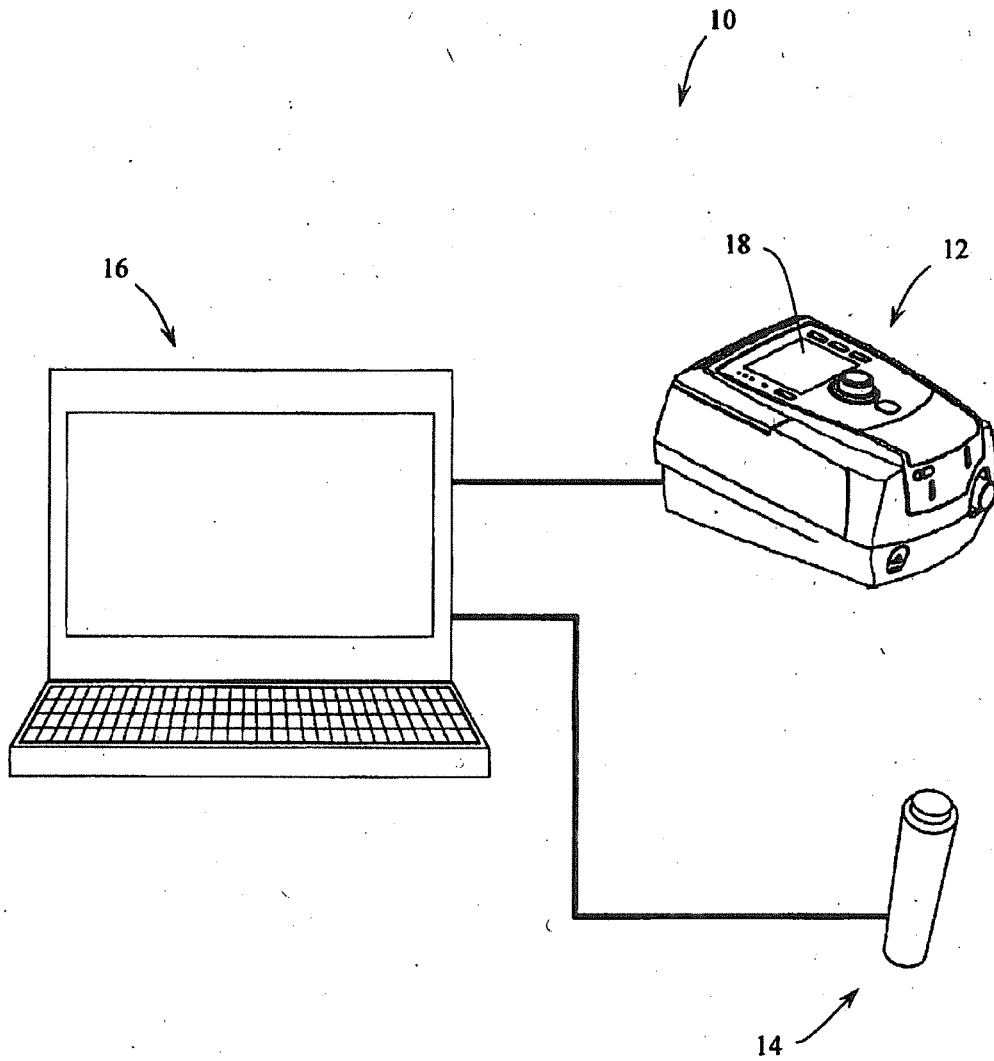


Figure 1

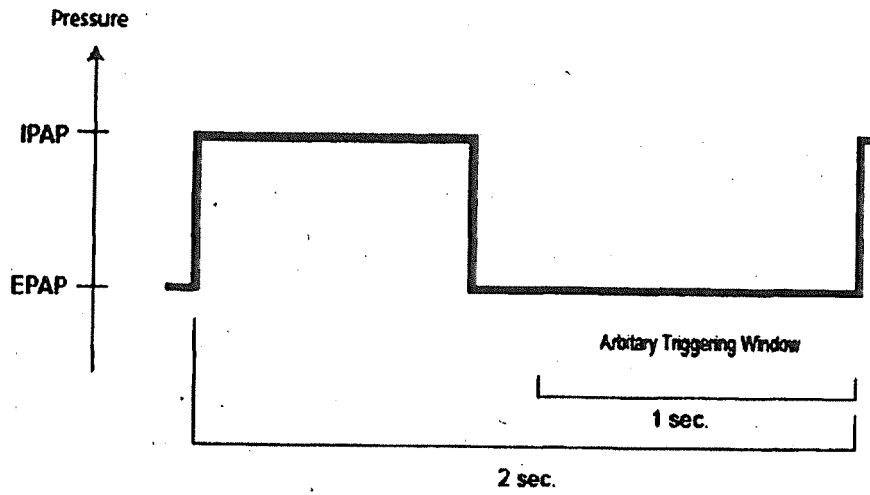


Figure 2a

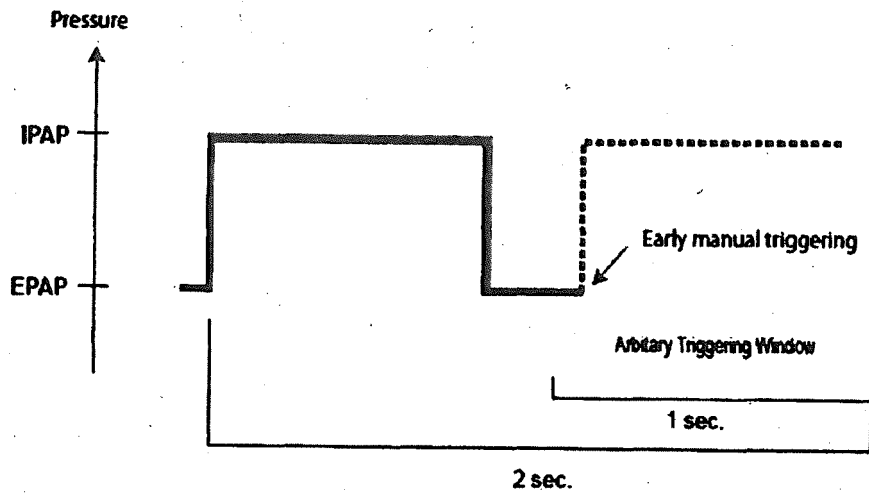


Figure 2b

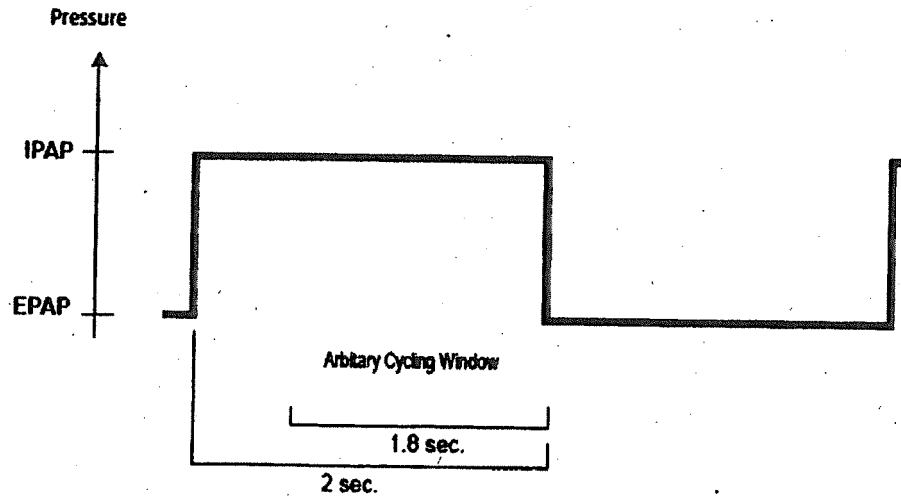


Figure 3a

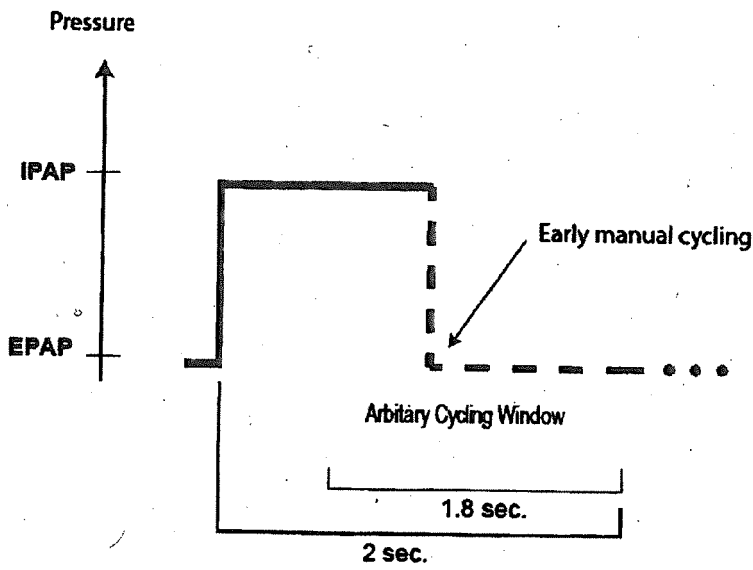


Figure 3b

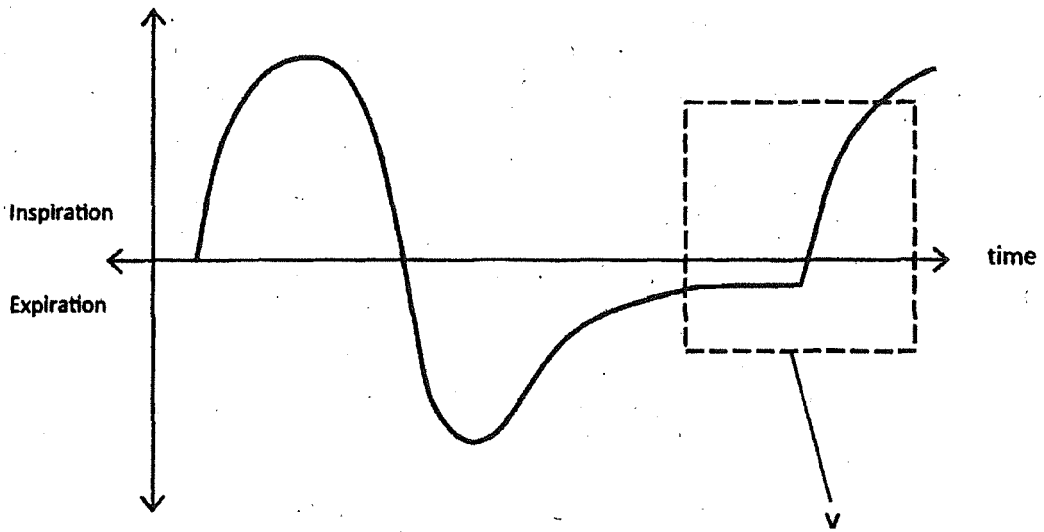


Figure 4

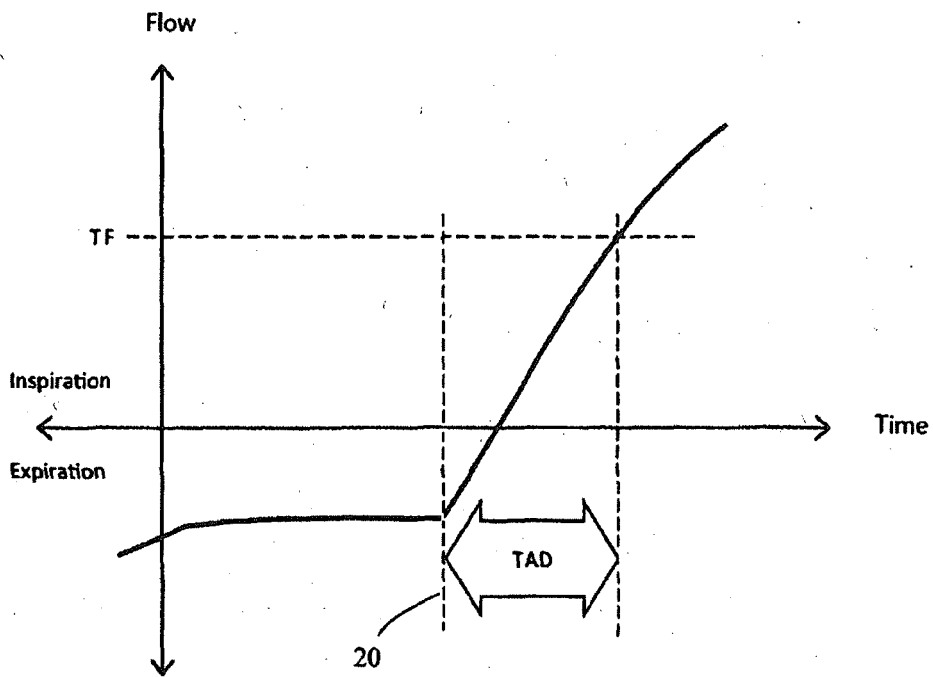


Figure 5

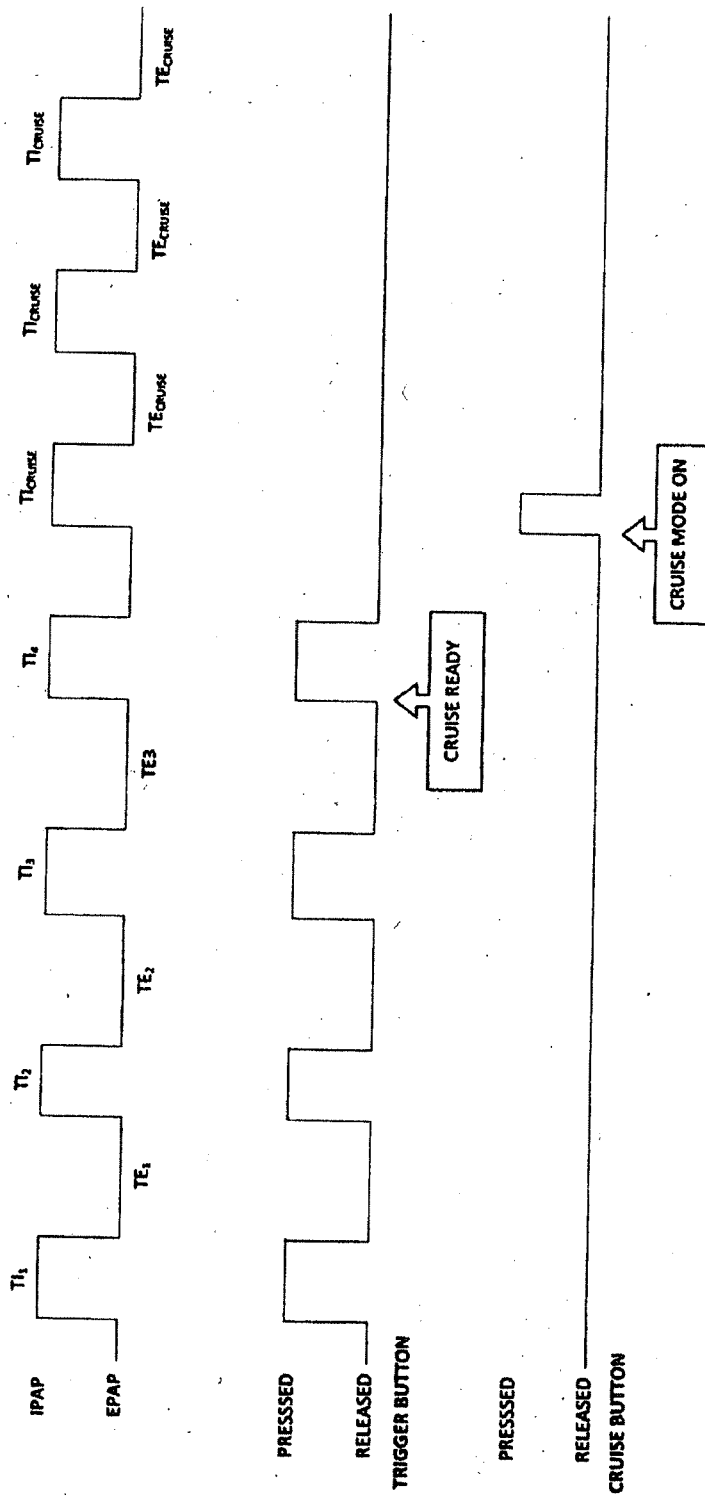


Figure 6

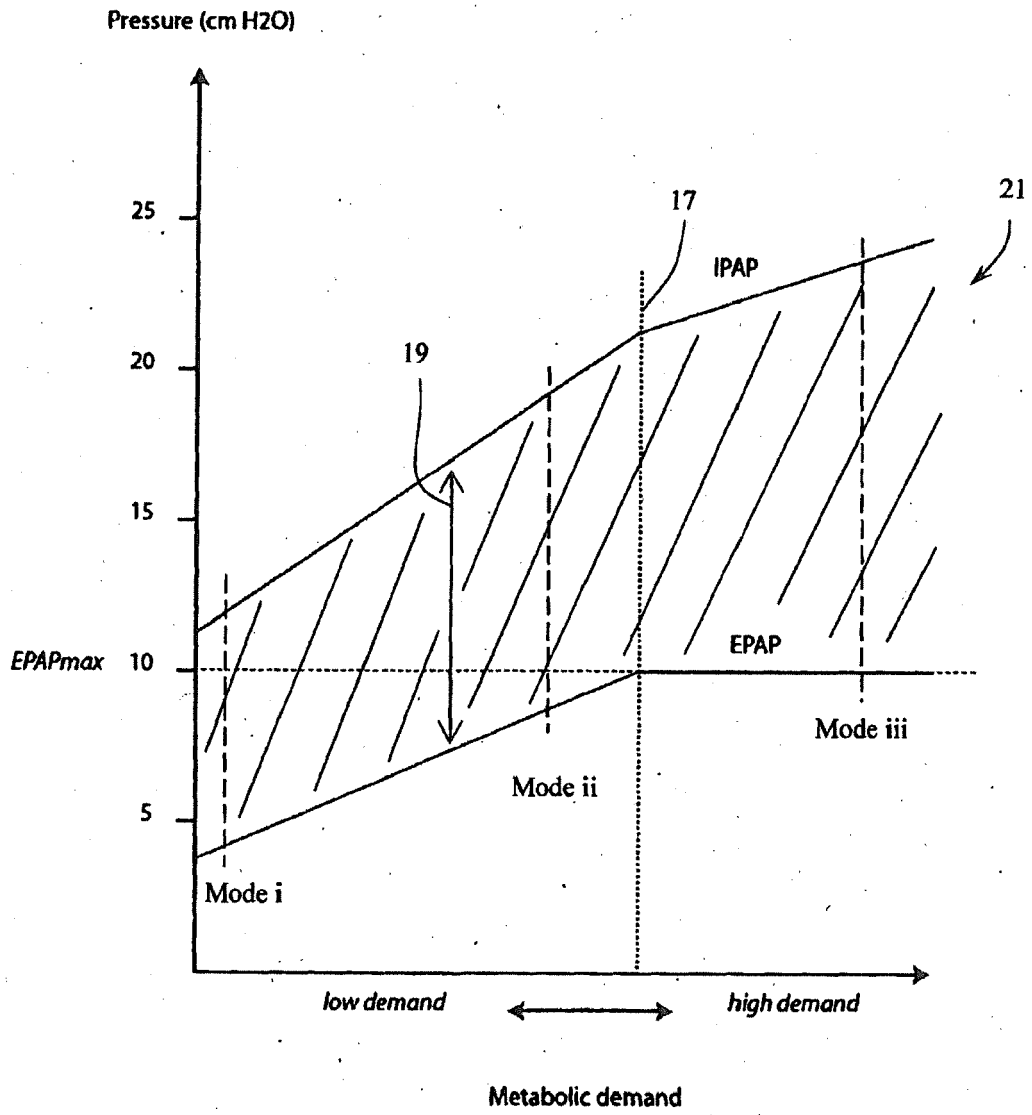


Figure 7A

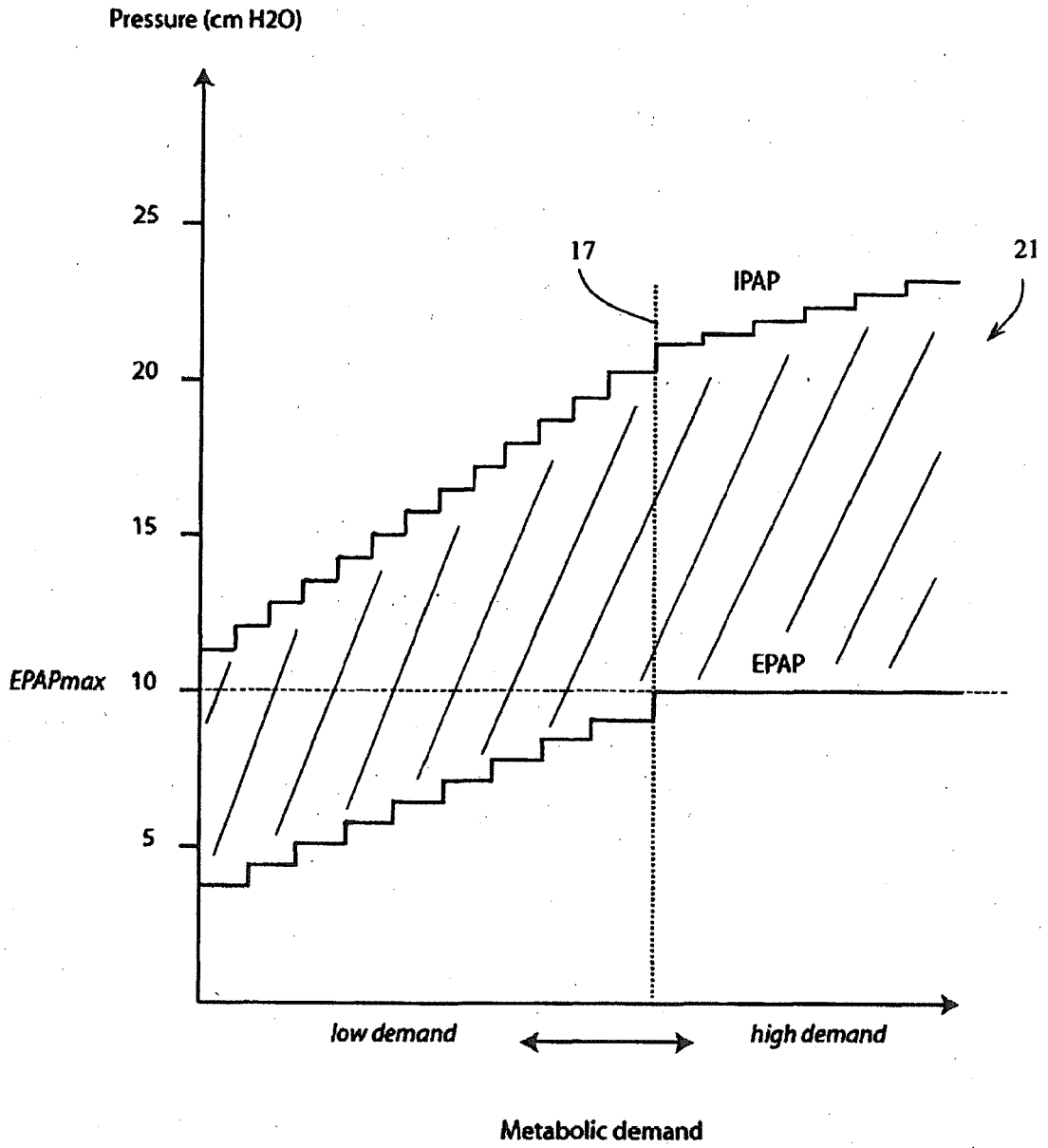


Figure 7B

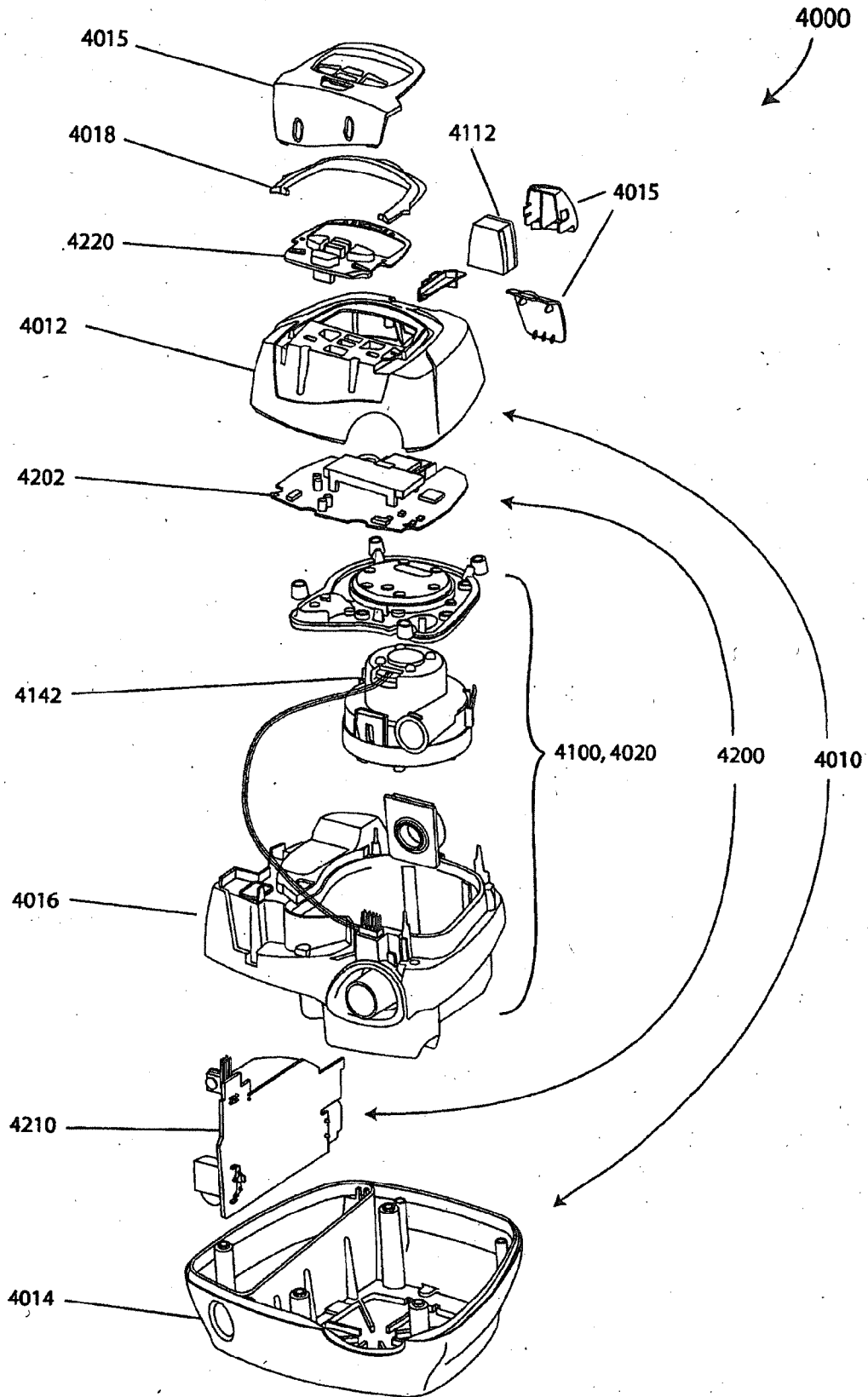


Fig. 8a

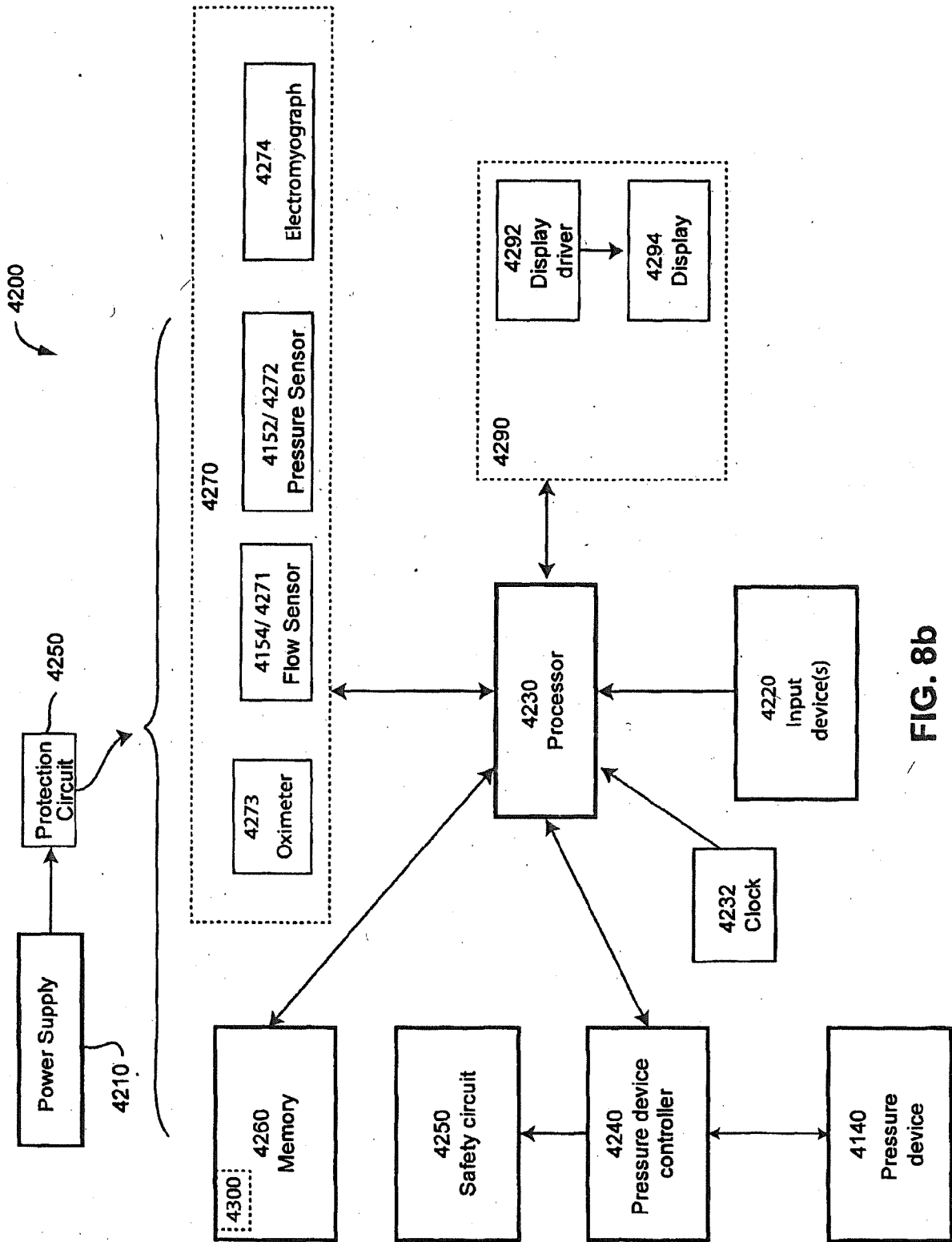


FIG. 8b

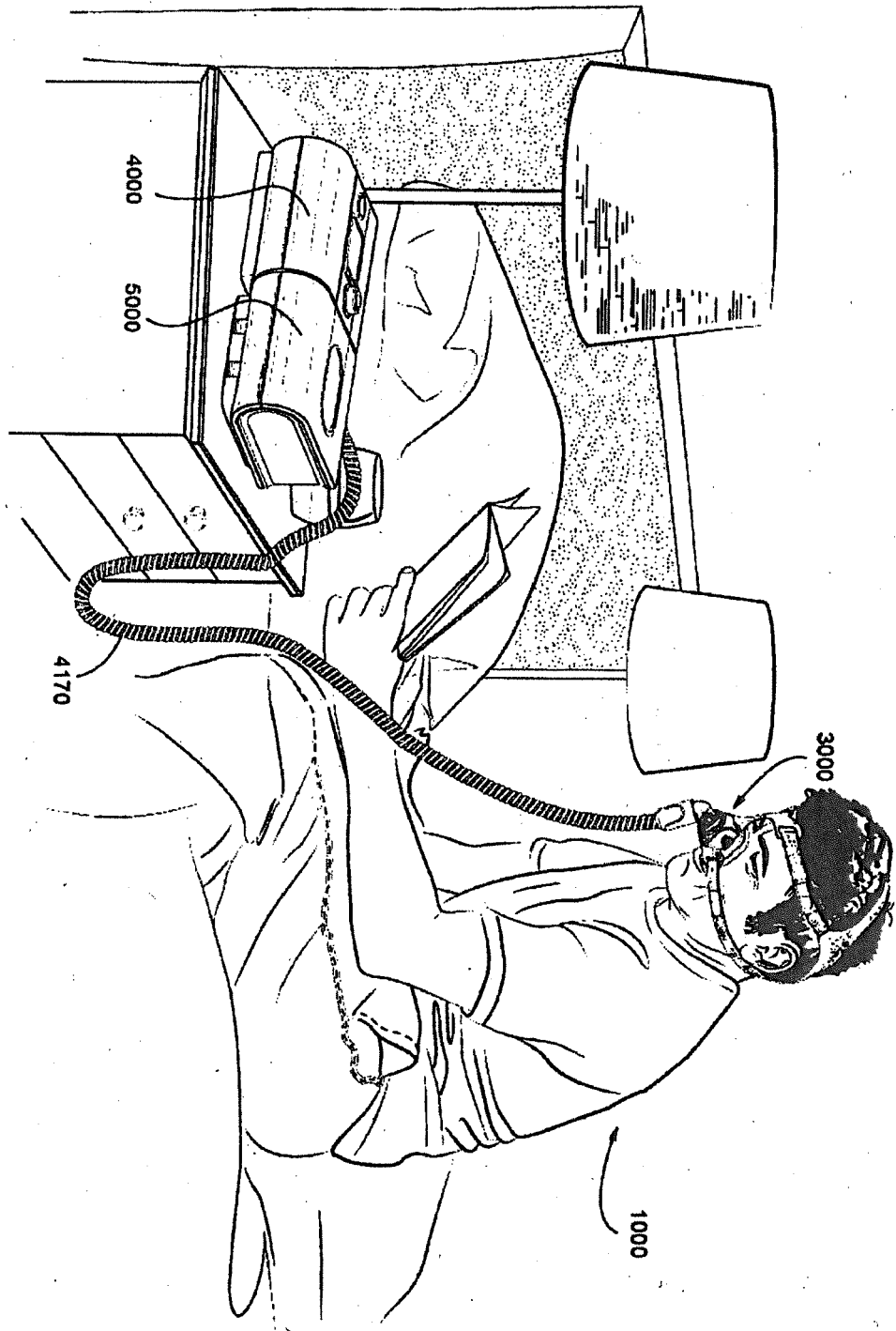


Fig 9

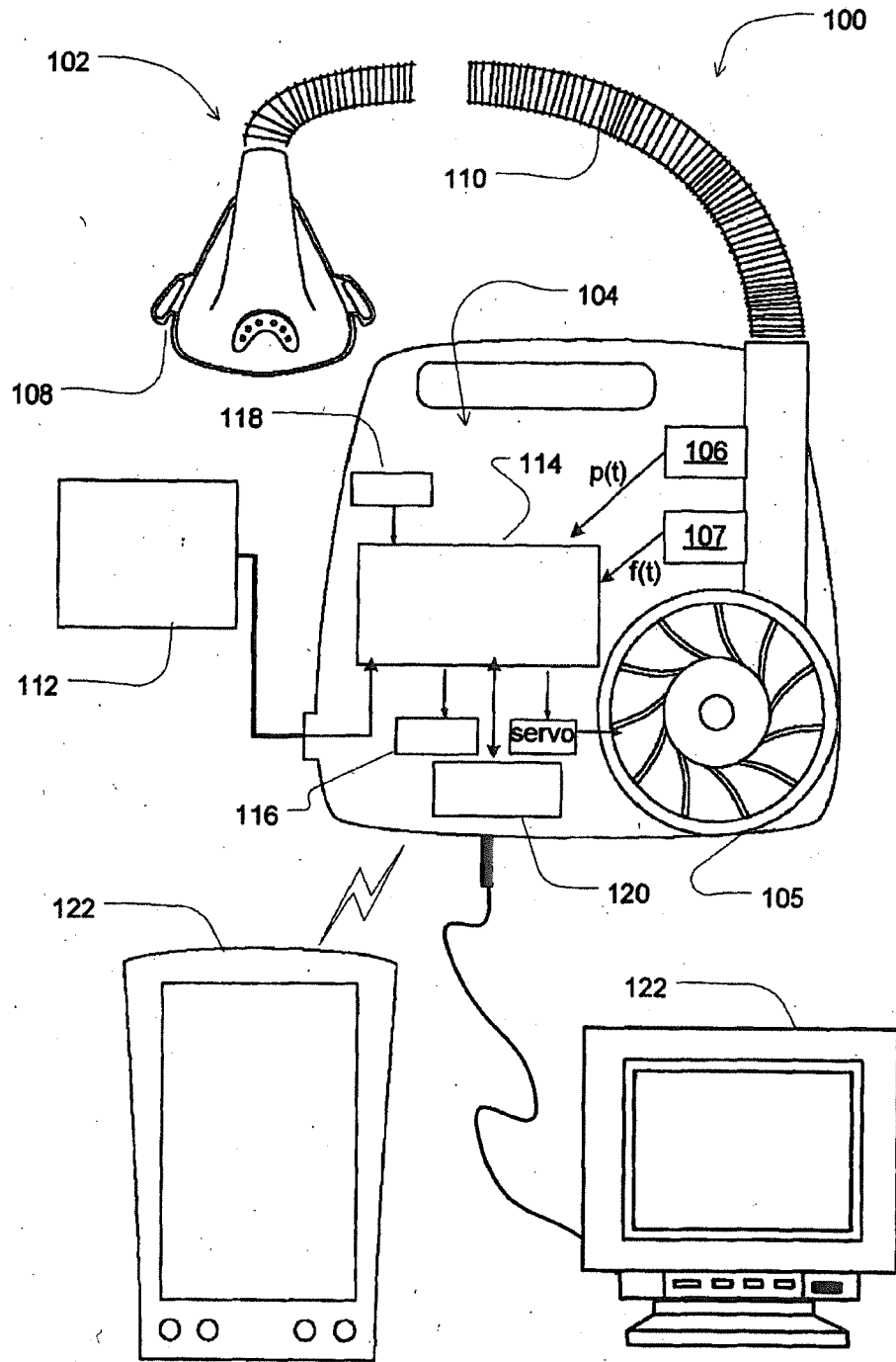
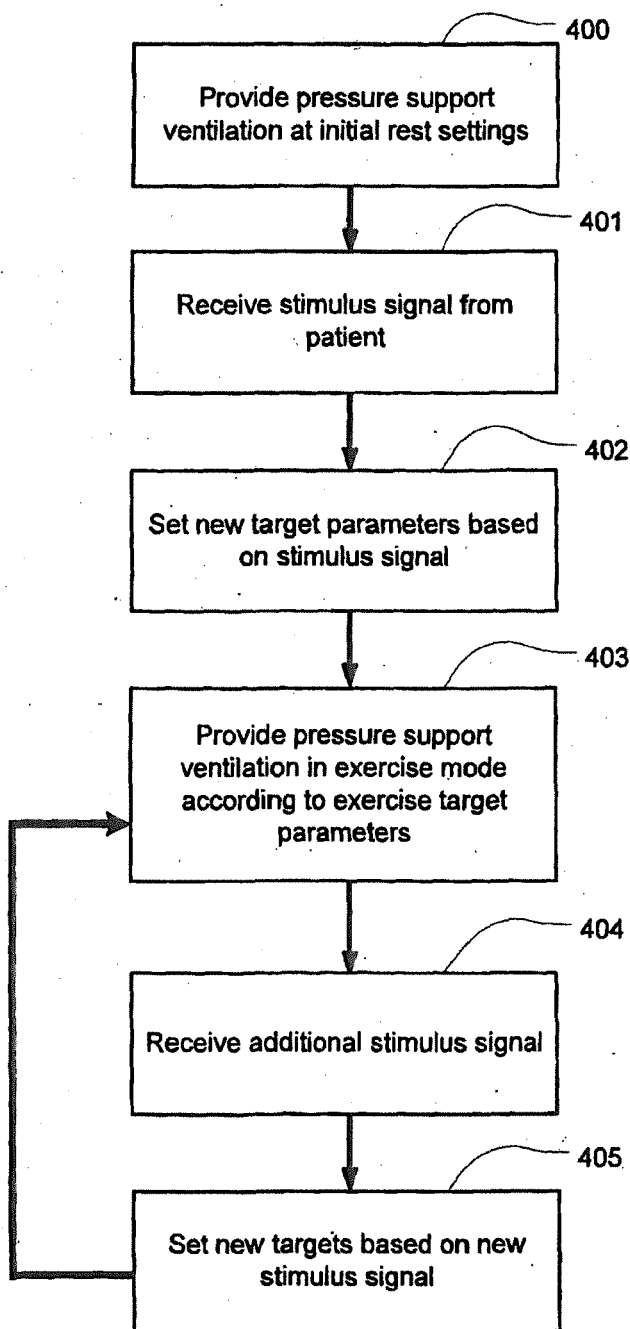


Fig. 10



**Fig. 11**

**REFERENCES CITED IN THE DESCRIPTION**

*This list of references cited by the applicant is for the reader's convenience only. It does not form part of the European patent document. Even though great care has been taken in compiling the references, errors or omissions cannot be excluded and the EPO disclaims all liability in this regard.*

**Patent documents cited in the description**

- AU 2011904599 [0001]
- AU 2012902501 [0001]
- AU 2012902693 [0001]
- US 6532957 B [0154]
- US 6845773 B [0154]
- US 6951217 B [0154]
- AU 2005001543 W [0155]
- WO 2006037184 A [0155]
- AU 1996000218 W [0155]
- WO 1996032055 A [0155]
- AU 1998000358 W [0157]
- WO 1998052467 A [0157]

**Non-patent literature cited in the description**

- **PESLIN et al.** Respiratory mechanics studied by forced oscillations during artificial ventilation. *EUR RESPIR J*, 1993, vol. 6, 772-784 [0108]

专利名称(译)	用于为患者提供通气的装置		
公开(公告)号	<a href="#">EP3245945A2</a>	公开(公告)日	2017-11-22
申请号	EP2017171378	申请日	2012-11-07
[标]申请(专利权)人(译)	雷斯梅德有限公司		
申请(专利权)人(译)	瑞思迈有限公司		
当前申请(专利权)人(译)	瑞思迈有限公司		
[标]发明人	SCHINDHELM KLAUS HENRY MALOUF GORDON JOSEPH FARRUGIA STEVEN PAUL DENNIS CLANCY JOHN BERTHON JONES MICHAEL BASSIN DAVID JOHN TESCHLER HELMUT		
发明人	SCHINDHELM, KLAUS HENRY MALOUF, GORDON JOSEPH FARRUGIA, STEVEN PAUL DENNIS, CLANCY JOHN BERTHON-JONES, MICHAEL BASSIN, DAVID JOHN TESCHLER, HELMUT		
IPC分类号	A61B5/00 A61B5/08 A61M16/00 A61M16/16 A61M16/10		
CPC分类号	A61M16/0006 A61M16/0051 A61M16/0069 A61M16/024 A61M16/107 A61M16/1075 A61M16/16 A61M2016/0027 A61M2016/0036 A61M2016/0039 A61M2205/502 A61M2230/205 A61B5/0205 A61B5 /024 A61B5/0488 A61B5/0816 A61B5/085 A61B5/087 A61B5/14551 A61B5/4836 A61B5/4866 A61M2016/0018 A61M2016/0033		
优先权	2011904599 2011-11-07 AU 2012902501 2012-06-15 AU 2012902693 2012-06-26 AU PCT/AU2012/001367 2012-11-07 WO		
其他公开文献	EP3245945A3		
外部链接	<a href="#">Espacenet</a>		

#### 摘要(译)

本技术涉及一种为患者提供通气的装置。特别地，本技术涉及改变呼吸机参数以匹配改变的患者代谢需求。

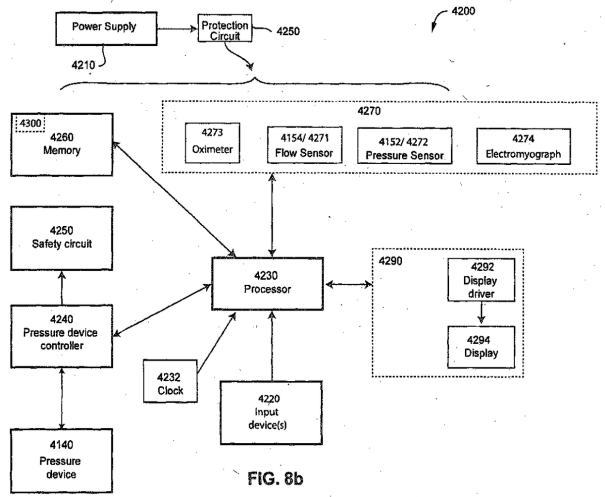


FIG. 8b