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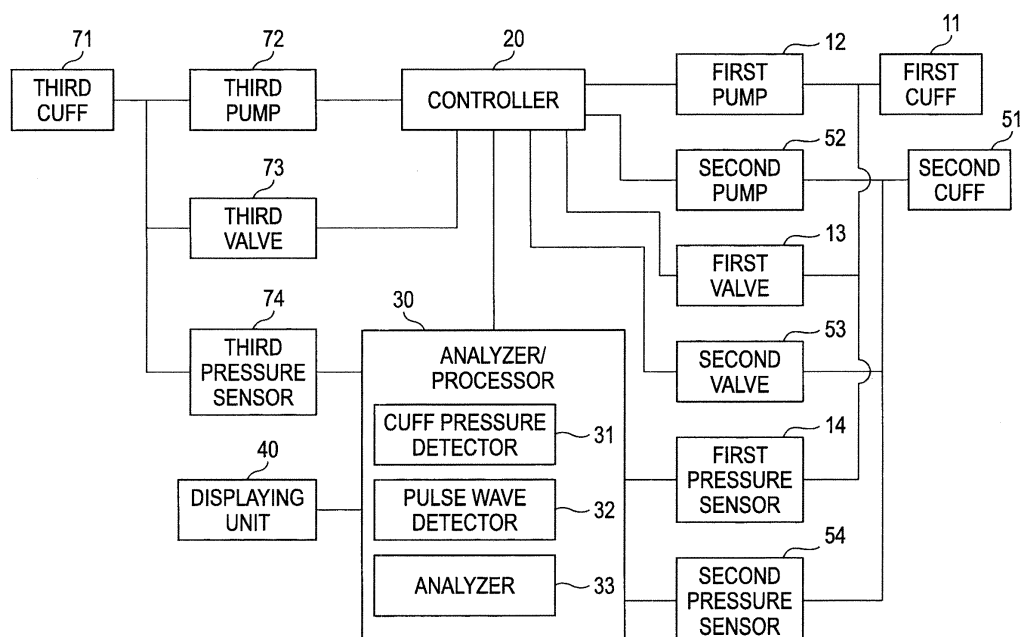
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(54) **Apparatus for evaluating vascular endothelial function**

(57) An apparatus for evaluating a vascular endothelial function includes a first cuff wrapped around one of right and left upper or lower limbs of a subject, a second cuff wrapped around the one of the right and left upper or lower limbs, a third cuff which is to be wrapped around another one of the right and left upper or lower limbs, a cuff pressure controller which controls pressures that are

applied to the first cuff, the second cuff and the third cuff, respectively, a cuff pressure detector which detects cuff pressures in the second cuff and the third cuff, a pulse wave detector which detects respective pulse waves at the second cuff and the third cuff from outputs of the pressure sensors.

FIG. 1



Description

BACKGROUND

[0001] The present invention relates to an apparatus for evaluating a vascular endothelial function in which avascularization is performed by using a cuff, a pulse wave is detected before and after the avascularization is detected, and a vascular endothelial function is evaluated based on the detected pulse waves.

[0002] The assignees of the present application have filed patent applications on apparatuses for evaluating a vascular endothelial function which, similarly with the above, use cuffs, and in which accurate evaluation similar to that obtained in a measurement using an ultrasonic echo system is enabled without using an ultrasonic echo system or the like (see JP-A-2009-273870 and JP-A-2011-056200).

[0003] In the apparatuses disclosed in the literatures, a vascular endothelial function is evaluated by comparing pulse waves before and after avascularization in place of a measurement in which the change of the vessel diameter before and after avascularization is measured by using an ultrasonic echo system.

[0004] According to the apparatuses for evaluating a vascular endothelial function disclosed in JP-A-2009-273870 and JP-A-2011-056200, accurate evaluation of a vascular endothelial function is enabled, but there may be a risk that the amplitude of a pulse wave is varied by influence of respiration and autonomic nerves in addition to an expansion of the vessel diameter caused by avascularization.

[0005] The invention has been conducted in view of the present status of an apparatus for evaluating a vascular endothelial function which uses cuffs. It is an object of the invention to provide an apparatus for evaluating a vascular endothelial in which accurate evaluation of a vascular endothelial function is enabled without being influenced by respiration and autonomic nerves.

SUMMARY

[0006] In one of its aspects, the apparatus for evaluating a vascular endothelial function of the invention is characterized in that the apparatus includes: a first cuff which is to be wrapped around one of right and left upper or lower limbs of a subject; a second cuff which is to be wrapped around one of the right and left upper or lower limbs, the one limb being to be wrapped by the first cuff; a third cuff which is to be wrapped around another one of the right and left upper or lower limbs, the other one limb being opposite to the one limb around which the first cuff and the second cuff are to be wrapped; a cuff pressure controller which controls pressures that are applied to the cuffs, respectively; a cuff pressure detector which, from an output of a pressure sensor connected to the second cuff, and an output of a pressure sensor connected to the third cuff, detects cuff pressures in the respec-

tive cuffs; a pulse wave detector which detects respective pulse waves from outputs of the pressure sensors; and an analyzer which analyzes the detected pulse waves to evaluate a vascular endothelial function, the cuff pressure controller controls the cuff pressure of the first cuff to avascularize the upper or lower limb around which the first cuff is wrapped, for a predetermined time period, the pulse wave detector detects a pulse wave corresponding to the second cuff, and a pulse wave corresponding to the third cuff, before and after the avascularization in a state where the cuff pressures of the second and third cuffs are controlled to respective predetermined pressure by the cuff pressure controller, and the analyzer corrects the pulse waves corresponding to the second cuff and detected before and after the avascularization, by the pulse waves corresponding to the third cuff and detected before and after the avascularization, and evaluates the endothelial function based on the corrected pulse waves corresponding to the second cuff.

[0007] In another of its aspects, the apparatus for evaluating a vascular endothelial function of the invention is characterized in that the apparatus includes: a second cuff which is to be wrapped around one of right and left upper or lower limbs of a subject; a third cuff which is to be wrapped around another one of the right and left upper or lower limbs, the other one limb being opposite to the one limb around which the second cuff is to be wrapped; a cuff pressure controller which controls pressures that are applied to the cuffs, respectively; a cuff pressure detector which, from an output of a pressure sensor connected to the second cuff, and an output of a pressure sensor connected to the third cuff, detects cuff pressures in the respective cuffs; a pulse wave detector which detects respective pulse waves from outputs of the pressure sensors; and an analyzer which analyzes the detected pulse waves to evaluate a vascular endothelial function, the cuff pressure controller controls the cuff pressure of the second cuff to avascularize the upper or lower limb around which the second cuff is wrapped, for a predetermined time period, the pulse wave detector detects a pulse wave corresponding to the second cuff, and a pulse wave corresponding to the third cuff, before and after the avascularization in a state where the cuff pressures of the second and third cuffs are controlled to respective predetermined pressures by the cuff pressure controller, and the analyzer corrects the pulse waves corresponding to the second cuff and detected before and after the avascularization, by the pulse waves corresponding to the third cuff and detected before and after the avascularization, and evaluates the vascular endothelial function based on the corrected pulse waves corresponding to the second cuff.

[0008] The apparatus for evaluating a vascular endothelial function of the invention may also be characterized in that the pulse waves handled in the analyzer are pulse wave indexes, and the pulse wave indexes are a parameter indicating a feature of a pulse wave.

[0009] The apparatus for evaluating a vascular en-

dothelial function of the invention may be characterized in that the correction corrects a result of a comparison between the pulse wave indexes corresponding to the second cuff and detected before and after the avascularization.

[0010] The apparatus for evaluating a vascular endothelial function of the invention may be characterized in that the comparison result is ratios of the pulse wave indexes of the second cuff and the third cuff before and after the avascularization, and the correction corrects the ratio of the pulse wave indexes corresponding to the second cuff by using the ratio of the pulse wave indexes corresponding to the third cuff.

[0011] The apparatus for evaluating a vascular endothelial function of the invention may be characterized in that the comparison and the correction are performed by using values of the pulse wave indexes corresponding to the second cuff or the third cuff, the values being obtained at a required timing, and values of the pulse wave indexes corresponding to the third cuff or the second cuff, the values being obtained at the required timing.

[0012] The apparatus for evaluating a vascular endothelial function of the invention may be characterized in that the comparison and the correction are performed by using values of the pulse wave indexes corresponding to the third cuff, and values of the pulse wave indexes corresponding to the second cuff and equal to the values of the pulse wave indexes corresponding to the third cuff.

[0013] The apparatus for evaluating a vascular endothelial function of the invention may be characterized in that the pulse wave indexes are a maximum value of a pulse wave amplitude, or a mean value in the vicinity of the maximum value.

[0014] The apparatus for evaluating a vascular endothelial function of the invention may be characterized in that the analyzer further performs a process of obtaining a systolic blood pressure and a diastolic blood pressure, and dividing an amplitude of the detected pulse wave by a difference between the systolic blood pressure and the diastolic blood pressure, thereby obtaining a compliance of a blood vessel.

[0015] According to the apparatus for evaluating a vascular endothelial function of the invention, the pulse waves corresponding to the second cuff and detected before and after the avascularization are corrected by those corresponding to the third cuff and detected before and after the avascularization, and the vascular endothelial function is evaluated based on the corrected pulse waves corresponding to the second cuff. Therefore, the vascular endothelial function can be accurately evaluated.

[0016] Namely, the pulse waves corresponding to the second cuff are presumed to contain an influence caused by an expansion of the vessel diameter due to the avascularization, and influences of respiration and autonomic nerves, and by contrast those corresponding to the third cuff are presumed to contain influences of respiration and autonomic nerves. When the pulse waves corre-

sponding to the second cuff and containing an influence caused by an expansion of the vessel diameter due to the avascularization, and influences of respiration and autonomic nerves are corrected by those corresponding to the third cuff and containing influences of respiration and autonomic nerves, therefore, it is possible to take out only information relating to the expansion of the vessel diameter due to the avascularization. Therefore, it is expected to accurately evaluate a vascular endothelial function without being influenced by respiration and autonomic nerves.

BRIEF DESCRIPTION OF DRAWINGS

[0017]

Fig. 1 is a block diagram of an apparatus for evaluating a vascular endothelial function of an embodiment of the invention.

Fig. 2 is a diagram illustrating a state where cuffs of the apparatus for evaluating a vascular endothelial function of the embodiment of the invention are attached to the body.

Figs. 3A to 3C are views showing in time series a first example of avascularization and pulse wave measurement in operation of the apparatus for evaluating a vascular endothelial function of the embodiment of the invention.

Fig. 4 is a flowchart illustrating the operation of avascularization and pulse wave measurement in operation of the apparatus for evaluating a vascular endothelial function of the embodiment of the invention. Figs. 5A to 5C are views showing an example of a statistical process performed by the apparatuses for evaluating a vascular endothelial function of the embodiment of the invention.

Figs. 6A to 6C are views showing in time series a second example of avascularization and pulse wave measurement in operation of the apparatus for evaluating a vascular endothelial function of the embodiment of the invention.

Figs. 7A to 7C are views showing in time series a third example of avascularization and pulse wave measurement in operation of the apparatus for evaluating a vascular endothelial function of the embodiment of the invention.

Figs. 8A to 8D are views showing in time series a fourth example of avascularization and pulse wave measurement in operation of the apparatus for evaluating a vascular endothelial function of the embodiment of the invention.

DETAILED DESCRIPTION OF EMBODIMENTS

[0018] Fig. 1 is a block diagram of an apparatus for evaluating a vascular endothelial function of an embodiment of the invention. The apparatus includes a first cuff 11, a second cuff 51, and a third cuff 71. A first pump 12,

a first valve 13, and a first pressure sensor 14 are connected to the first cuff 11. A second pump 52, a second valve 53, and a second pressure sensor 54 are connected to the second cuff 51. A third pump 72, a third valve 73, and a third pressure sensor 74 are connected to the third cuff 71. The apparatus further includes a controller 20, an analyzer/processor 30, and a displaying unit 40. The analyzer/processor 30 is connected to the controller 20, and the displaying unit 40 is connected to the analyzer/processor 30. The first pump 12, the second pump 52, the third pump 72, the first valve 13, the second valve 53, and the third valve 73 are connected to the controller 20, and the first pressure sensor 14, the second pressure sensor 54, and the third pressure sensor 74 are connected to the analyzer/processor 30.

[0019] The first cuff 11 is to be wrapped around a first portion such as an upper or lower limb of the body of the subject, and used for applying a pressure for avascularization on the portion around which the cuff is wrapped. The second cuff 51 is to be wrapped around a second portion such as the upper or lower limb of the body of the subject on the side where the first cuff 11 is wrapped, and used for applying a pressure for detecting a pulse wave of the portion around which the cuff is wrapped. In a measurement, as shown in Fig. 2, for example, the first cuff 11 and the second cuff 51 are wrapped around an arm portion of the arm, and the second cuff 51 is preferably wrapped around a portion which is on the upstream side (the side which is closer to the heart) of the first cuff 11. The third cuff 71 is to be wrapped around a portion in the upper and lower limbs of the body, on the side (left or right side) which is different from the side (right or left side) around which the first cuff 11 and the second cuff 51 are wrapped, and used for applying a pressure for detecting a pulse wave of the portion around which the cuff is wrapped. In a measurement, in the case where the first cuff 11 and the second cuff 51 are wrapped around the left arm of the body as shown in Fig. 2, for example, the third cuff 71 is wrapped around the side of the right arm (side of the upper and lower limbs which is not avascularized).

[0020] The first pump 12 feeds the air into the first cuff 11 under the control of the controller 20. The first valve 13 switches non-discharging/discharging of the air in the first cuff 11 under the control of the controller 20. The second pump 52 feeds the air into the second cuff 51 under the control of the controller 20. The second valve 53 switches non-discharging/discharging of the air in the second cuff 51 under the control of the controller 20. The third pump 72 feeds the air into the third cuff 71 under the control of the controller 20. The third valve 73 switches non-discharging/discharging of the air in the third cuff 71 under the control of the controller 20. The controller 20 constitutes the cuff pressure controller which controls pressurization and depressurization of the first cuff 11, the second cuff 51, and the third cuff 71.

[0021] The first pressure sensor 14 outputs a signal corresponding to the pressure in the first cuff 11, the sec-

ond pressure sensor 54 outputs a signal corresponding to the pressure in the second cuff 51, and the third pressure sensor 74 outputs a signal corresponding to the pressure in the third cuff 71. The analyzer/processor 30 controls the whole apparatus, is configured by, for example, a computer, and includes a cuff pressure detector 31, a pulse wave detector 32, and an analyzer 33. In the embodiment, for the sake of convenience, the controller 20 which controls the first cuff 11, the second cuff 51, and the third cuff 71, and the analyzer/processor 30 which performs analysis and processing are commonly used for the cuffs. Alternatively, they may be disposed for each of the cuffs.

[0022] The cuff pressure detector 31 detects the respective cuff pressures of the first, second, and third cuffs 11, 51, 71 from outputs of the first, second, and third pressure sensors 14, 54, 74. The pulse wave detector 32 detects pulse waves from the outputs of the second pressure sensor 54 and the third pressure sensor 74. The analyzer 33 calculates a systolic blood pressure and a diastolic blood pressure based on the detected pulse waves, and, as described later, analyzes pulse waves before and after the avascularization to evaluate a vascular endothelial function. The displaying unit 40 displays a result of the evaluation of the vascular endothelial function, the blood pressure value, and the like.

[0023] The controller 20 drives the first, second, and third pumps, and the first, second, and third valves to control the cuff pressures of the first, second, and third cuffs to a predetermined value. For example, the cuff pressures of the first cuff 11, the second cuff 51, and the third cuff 71 are changed as shown in Fig. 3A. Namely, avascularization is performed by using the first cuff 11 during a pressurization (avascularization) period T, and the pulse wave is measured before and after the pressurization period T, i.e., during measurement periods Tp and Ta by using the second cuff 51 and the third cuff 71. For example, the pressurization period T may be set to about five minutes, and the measurement periods Tp and Ta may be set to a time period which is required for usual blood pressure measurement. During the pressurization period T, the output of the first pressure sensor 14 is monitored, and avascularization is performed at a pressure which is a sum of the systolic blood pressure and a predetermined pressure (for example, 50 mmHg). In the measurement periods Tp and Ta, the output of the second pressure sensor 54 is monitored in the second cuff 51, that of the third pressure sensor 74 is monitored in the third cuff 71, the cuff pressures which are higher than the systolic blood pressure are gradually lowered, and pulse waves respectively corresponding to the cuffs are measured.

[0024] The apparatus for evaluating a vascular endothelial function can perform processing shown in, for example, the flowchart of Fig. 4. As described above, the first cuff 11 is wrapped around the left arm of the body of the subject as shown in, for example, Fig. 2, the second cuff 51 is wrapped around the left arm of the subject, and

on the upstream side of the first cuff 11, the third cuff 71 is wrapped around the right arm of the body of the subject, and then the measurement is started. Under the control of the controller 20, the air is sent in a state where the second valve 53 is closed, from the second pump 52 to the second cuff 51, and, at the same time, from the third pump 72 to the third cuff 71 in a state where the third valve 73 is closed, to raise the cuff pressures (S11).

[0025] When the cuff pressures reaches a predetermined value, the air supplies from the second pump 52 and the third pump 72 are stopped, and the second valve 53 and the third valve 73 are controlled, whereby the cuff pressures are gradually lowered (S12).

[0026] During the process of lowering the cuff pressures, the cuff pressure detector 31 detects the cuff pressures from the outputs of the second pressure sensor 54 and the third pressure sensor 74, and the pulse wave detector 32 detects the pulse waves for each beat. Based on the cuff pressures and the pulse waves, the analyzer 33 obtains the values of the respective pulse wave indexes (S13). In the embodiment, the respective maximal pulse wave amplitudes are set as the pulse wave indexes. The maximal pulse wave amplitudes are obtained by statistically processing the pulse waves which are obtained in the measurement period T_p . The pulse wave in the measurement period T_p obtained by the second pressure sensor 54 is as shown in Fig. 3B, and the maximal pulse wave amplitude A_c is obtained as the value of the pulse wave index.

[0027] The blood pressure at the timing when the pulse wave shows the maximal amplitude in the measurement period T_p is the mean blood pressure. In the case where the mean blood pressure is previously known, therefore, pressurization to a pressure which is equal to or higher than the mean blood pressure is not necessary in order to obtain the maximal pulse wave, and the burden on the subject is reduced.

[0028] Similarly, the pulse wave in the measurement period T_p obtained by the third pressure sensor 74 is as shown in Fig. 3C, and the maximal pulse wave amplitude A_o is obtained in a similar manner as the maximal pulse wave amplitude A_c which is obtained from the pulse wave acquired by the second pressure sensor 54. In addition to the maximal pulse wave amplitude, a value in the vicinity of the maximal pulse wave amplitude (including a mean value), the velocity (first order differential of the pulse wave), the area, the acceleration (second order differential of the pulse wave), the time period until a peak, and the like may be used as the pulse wave index.

[0029] Next, the pressurization period T for avascularization when, in a state where the first valve 13 is closed under the control of the controller 20, the air is sent from the first pump 12 to the first cuff 11 to raise the cuff pressure, and avascularization is performed at a pressure which is a sum of the systolic blood pressure and the predetermined pressure (for example, 50 mmHg) is realized (S14). After five minutes, the first valve 13 is opened to release the cuff pressure, whereby the cuff

pressure is lowered to a pressure which is equal to or lower than the systolic blood pressure (S15).

[0030] Thereafter, a state where the second valve 53 and the third valve 73 are closed is promptly set, the air is sent from the second pump 52 to the second cuff 51, and the air is sent from the third pump 72 to the third cuff 71, so that to the pressures of the cuffs are raised (S16). When the cuff pressures reach a predetermined value, the pressures of the second cuff 51 and the third cuff 71 are gradually lowered in a similar manner as described above (S17).

[0031] During the process of lowering the cuff pressures, the cuff pressures and the pulse waves for each beat are detected in a similar manner as step S13, and the analyzer 33 obtains the maximal pulse wave amplitudes B_c and B_o as the values of the pulse wave indexes from the cuff pressures and the pulse waves (S18).

[0032] Then, a result of comparison of the maximal pulse wave amplitudes A_c and B_c of the avascularization side is corrected by using that of comparison of the maximal pulse wave amplitudes A_o and B_o of the non-vascularization side (S19). Each of the comparisons can be performed by obtaining a result of a division of the maximal pulse wave amplitude B_c (B_o) by the maximal pulse wave amplitude A_c (A_o). Therefore, the comparison result of the avascularization side is (B_c/A_c) , and that of the non-vascularization side is (B_o/A_o) . The correction may be performed by dividing (B_c/A_c) of the comparison result of the avascularization side by (B_o/A_o) of the comparison result of the non-vascularization side, or by subtracting (B_o/A_o) of the comparison result of the non-vascularization side from (B_c/A_c) of the comparison result of the avascularization side.

[0033] The corrected maximal pulse wave amplitude ratio of the avascularization side is displayed together with the systolic blood pressure and the diastolic blood pressure, on the displaying unit 40 (S20). The vascular endothelial function is evaluated by the corrected maximal pulse wave amplitude values of the avascularization side which are displayed.

[0034] In the above, the comparison results are obtained in first. Alternatively, the correction may be performed in first. For example, the representative pulse wave amplitude A_c (B_c) of the avascularization side may be divided or subtracted by the representative pulse wave amplitude A_o (B_o) of the non-vascularization side to obtain the corrected pulse wave amplitude (for example, A_b) before avascularization and the corrected pulse wave amplitude (for example, B_a) after avascularization, and (B_a/A_b) may be obtained by comparison.

[0035] The relationship between the pulse wave amplitude and the cuff pressure is not constant. Figs. 5A to 5C show the relationship between the cuff pressure and the pulse wave amplitude. Fig. 5A shows the pulse wave amplitude in the case where the cuff pressure is lowered at the rate of 5 mmHg per beat, and Figs. 5B and 5C show the pulse wave amplitude in the case where the pressure reduction rate is increased. In the figures, the

cuff pressure and pulse wave amplitude at the start of the pressure reduction are different.

[0036] In Figs. 5B and 5C, the maximal pulse wave amplitudes are 3 mmHg and 2.8 mmHg, respectively, and the difference of 0.2 mmHg is produced. The analyzer 33 performs statistical processing in which the mean value of a predetermined number (for example, three) of pulse wave amplitudes in the vicinity of the maximal pulse wave amplitude is calculated among obtained pulse wave amplitudes. In the example, when the mean value of pulse wave amplitudes at three points is calculated, the average is 2.67 mmHg in Fig. 5B, and 2.64 mmHg in Fig. 5C. The difference can be reduced, and a value which is preferred as the maximal pulse wave amplitude can be obtained. In the embodiment, it is assumed that the value of the maximal pulse wave amplitude includes a value in the vicinity of the maximal pulse wave amplitude (including a mean value).

[0037] In the above, during the measurement periods T_p and T_a , the maximum value of the pulse wave amplitude corresponding to the second cuff 51 (hereinafter, the amplitude is referred to as the pulse wave amplitude of the second cuff 51) is obtained, also the maximum value of the pulse wave amplitude corresponding to the third cuff 71 (hereinafter, the amplitude is referred to as the pulse wave amplitude of the third cuff 71) is similarly obtained, and the values are used in the correction. In the measurement periods T_p and T_a , however, the time when the pulse wave amplitude of the second cuff 51 is maximum is not always identical with that when the pulse wave amplitude of the third cuff 71 is maximum. Therefore, the correction may be performed by obtaining the pulse wave amplitude of the third cuff 71 at the time when the pulse wave amplitude of the second cuff 51 is maximum (the times when A_c and B_c are attained in Fig. 3B). Similarly, the correction may be performed by obtaining the pulse wave amplitude of the second cuff 51 at the time when the pulse wave amplitude of the third cuff 71 is maximum (the times when A_o and B_o are attained in Fig. 3C). When the timing when the pulse wave is acquired in the avascularization side is coincident with that in the non-vascularization side as described above, it is possible to realize a more correct correction.

[0038] Before avascularization, the pulse wave amplitudes of the second cuff 51 and the third cuff 71 may be obtained at the same timing, and, after avascularization, the timing when the pulse wave amplitude of the third cuff 71 of the non-vascularization side after avascularization is equal to that of the third cuff 71 before avascularization may be obtained. Then, the pulse wave amplitude of the second cuff 51 of the avascularization side at this timing may be obtained, and used as a value (hereinafter, referred to as the representative value) to be used in the comparison.

[0039] As shown in Figs. 6A to 6C, during the measurement period T_p before avascularization, for example, the maximal pulse wave amplitude A_c is obtained as the representative value from the pulse wave of the second

cuff 51, and at the same time the pulse wave amplitude A_o is obtained as the representative value from the pulse wave of the third cuff 71 (time t_1). During the measurement period T_a after avascularization, then, the time is obtained when the pulse wave of the third cuff 71 having the same amplitude as the pulse wave amplitude A_o which is obtained before avascularization is acquired. For example, it is assumed that the pulse wave amplitude B_o which is identical in amplitude with the pulse wave amplitude A_o that is obtained before avascularization is acquired at time t_2 , and then the obtained pulse wave amplitude B_o is set as the representative value. It is assumed that the representative value of the second cuff 51 of the avascularization side after avascularization is the pulse wave amplitude B_c acquired at time t_2 . The representative values A_o and B_o of the non-vascularization side before and after avascularization are identical with each other. Therefore, the vascular endothelial function is evaluated by the comparison result B_c/A_c of the representative values of the avascularization side.

[0040] In the embodiment, the pulse wave amplitude is measured during the process of depressurizing the cuff pressure. Alternatively, the measurement may be performed during the process of pressurizing the cuff pressure.

[0041] Furthermore, the pulse wave amplitude for each beat may be measured in a state where the cuff pressure is kept constant (at a constant pressure). For example, the constant pressure may be about 20 mmHg.

[0042] The embodiment is configured so that avascularization is performed by the first cuff 11, and the pulse wave for each beat is measured by the second cuff 51. Alternatively, the first cuff 11 and the second cuff 51 may be configured as a single cuff. In the alternative, the configuration of Fig. 1 is modified so that the first cuff 11, the first pump 12, the first valve 13, and the first pressure sensor 14 are removed away, and the second cuff 51, the second pump 52, the second valve 53, and the second pressure sensor 54 are provided also with the function for avascularization. The third cuff 71, the third pump 72, the third valve 73, and the third pressure sensor 74 are not changed.

[0043] The operation of performing avascularization on the subject for a predetermined time as described above means the followings. Normal vascular endothelial cells are caused to produce vasodepressor materials such as nitric monoxide (NO) by stimulation due to a blood flow or medication. When the vascular endothelial function is lowered, the ability of producing the vasodepressor materials is lowered. With a measurement of the degree of vessel expansion due to avascularization, it is possible to evaluate the vascular endothelial function.

[0044] The relationships among the inner vascular pressure, the cuff pressure, and the pulse wave amplitude contained in the cuff pressure signal can be described as follows. First, it is known that, when the inner vascular pressure and the cuff pressure are equal to each other, the vascular compliance is maximum. When the

cuff pressure is equal to the mean blood pressure, the difference between the maximal and minimal blood pressures in a vessel, i.e., the vessel volumetric change due to the pulse pressure is maximum. In the measurement periods T_p and T_a before and after avascularization, therefore, the maximal pulse wave amplitudes A_c and B_c are measured by using the second cuff 51, and set as representative pulse wave amplitudes of the avascularization side, and the maximal pulse wave amplitudes A_o and B_o are measured by using the third cuff 71, and set as representative pulse wave amplitudes of the non-vascularization side.

[0045] Alternatively, the mean blood pressure may be previously measured, and the pulse wave amplitude at the application of the cuff pressure corresponding to the mean blood pressure may be set as the representative value. In any case, the representative value is obtained by applying statistical processing on the pulse wave amplitudes in the measurement periods T_p and T_a in which the second cuff 51 and the third cuff 71 are used.

[0046] In the above description, the measurement of the pulse wave amplitude by using the second cuff 51 and the third cuff 71 is performed one time respectively before and after the pressurization period T for avascularization. Alternatively, a plurality of measurements may be performed. In the alternative, the numbers of measurements before and after avascularization may be different from each other.

[0047] Figs. 7A to 7C show an example in which, in each of the measurement periods T_p and T_a , the pulse wave amplitude is measured two times. In this example, during the measurement period T_p shown in Fig. 7A, two pulse wave measurements are performed by using the second cuff 51, and the pulse wave detector 32 obtains measured-value groups X_{c1} and X_{c2} . The analyzer 33 performs statistical processing on the measured-value groups X_{c1} and X_{c2} to obtain representative values. In this example, maximal pulse wave amplitudes A_{c1} and A_{c2} are obtained as representative values as shown in Fig. 7B.

[0048] Similarly, during the measurement period T_p , two measurements are performed by using the third cuff 71, and the pulse wave detector 32 obtains measured-value groups X_{o1} and X_{o2} . The analyzer 33 performs statistical processing on the measured-value groups X_{o1} and X_{o2} to obtain representative values. In this example, maximal pulse wave amplitudes A_{o1} and A_{o2} are obtained as representative values as shown in Fig. 7C.

[0049] Also during the measurement period T_a shown in Fig. 7A, two measurements are performed by using the second cuff 51, and the pulse wave detector 32 obtains measured-value groups Y_{c1} and Y_{c2} . The analyzer 33 performs statistical processing on the measured-value groups Y_{c1} and Y_{c2} , and maximal pulse wave amplitudes B_{c1} and B_{c2} are obtained as representative values as shown in Fig. 7B.

[0050] Similarly, during the measurement period T_a shown in Fig. 7A, two measurements are performed by

using the third cuff 71, and the pulse wave detector 32 obtains measured-value groups Y_{o1} and Y_{o2} . The analyzer 33 performs statistical processing on the measured-value groups Y_{o1} and Y_{o2} , and maximal pulse wave amplitudes B_{o1} and B_{o2} are obtained as representative values as shown in Fig. 7C.

[0051] The analyzer 33 performs statistical processing for obtaining the respective mean values on the maximum pulse wave amplitudes A_{c1} and A_{c2} and maximum pulse wave amplitudes B_{c1} and B_{c2} , and the maximum pulse wave amplitudes A_{o1} and A_{o2} and maximum pulse wave amplitudes B_{o1} and B_{o2} which are obtained in the above-described processes, to obtain final representative values. By using the obtained representative values, the representative values of the avascularization side before and after avascularization are compared with each other, and a result of the comparison can be corrected by the representative values of the non-vascularization side before and after avascularization. As a result of the above-described measurements and processing, errors can be leveled, and accurate evaluation is enabled.

[0052] Other measurement technique and statistical processing will be described. The vessel expansion due to avascularization by the first cuff 11 and its release, i.e., the increase of the vessel diameter is gradually increased after the release of the avascularization to reach the peak after several tens of seconds, and thereafter is reduced for several minutes. Based on the peak, it is possible to evaluate the degree of vessel expansion. After avascularization using the first cuff 11, the maximum value of the pulse wave amplitude is measured several times by using the second cuff 51 and the third cuff 71, and a maximum one of the maximum values is set as the pulse wave amplitude in the vessel expansion, thereby obtaining the peak of the vessel expansion.

[0053] As shown in Fig. 8A, specifically, the measurement period T_a for measuring the pulse wave amplitude by using the second cuff 51 and the third cuff 71 is realized after the pressurization period T using the first cuff 11. In the example, in accordance with four measurements using the second cuff 51, measured-value groups Y_{c1} , Y_{c2} , Y_{c3} , and Y_{c4} are obtained as shown in Fig. 8C. In this case, the vessel diameter changes as shown Fig. 8B, and it is estimated that a peak P exists in the vicinity of the measured-value group Y_{c2} . The analyzer 33 performs statistical processing on the measured-value groups Y_{c1} , Y_{c2} , Y_{c3} , and Y_{c4} , and, as shown in Fig. 8C, obtains maximal pulse wave amplitudes B_{c1} , B_{c2} , B_{c3} , and B_{c4} as candidates for the representative value.

[0054] The analyzer 33 compares the levels of the maximal pulse wave amplitudes B_{c1} , B_{c2} , B_{c3} , and B_{c4} with one another, and selects the maximal pulse wave amplitude B_{c2} as the representative value.

[0055] Similarly, in accordance with four measurements using the third cuff 71, measured-value groups Y_{o1} , Y_{o2} , Y_{o3} , and Y_{o4} are obtained. The analyzer 33 performs statistical processing on the measured-value groups Y_{o1} , Y_{o2} , Y_{o3} , and Y_{o4} , and, as shown in Fig.

8D, obtains maximal pulse wave amplitudes Bo1, Bo2, Bo3, and Bo4 as candidates for the representative value.

[0056] The analyzer 33 compares the levels of the maximal pulse wave amplitudes Bo1, Bo2, Bo3, and Bo4 with one another, and selects the maximal pulse wave amplitude Bo2 as the representative value. The maximal pulse wave amplitude Bc2 which is maximum in the avascularization side is corrected by the maximal pulse wave amplitude Bo2 which is maximum in the non-vascularization side, and also the maximal pulse wave amplitude which is obtained by the measurement before the pressurization period T is corrected as described above. The analyzer 33 performs comparison by using the corrected results, and calculates a ratio of the correction results before and after the pressurization period T. The calculated result is displayed together with the obtained blood pressure value on the displaying unit 40. As described above, the ratio may be obtained in first, and then the comparison may be performed.

[0057] The analyzer 33 performs processing in which the vascular compliance is obtained, in addition to the processings in which a result of comparison of pulse waves, and blood pressures are obtained. The analyzer 33 divides the detected pulse wave amplitude by the difference (pulse pressure) between the systolic blood pressure and the diastolic blood pressure, to obtain the vascular compliance C. Although the phenomenon in which, when the inner vascular pressure and the cuff pressure are equal to each other, the vascular compliance is maximum is already known, the compliance which is to be obtained in this case is not restricted to a value obtained when the inner vascular pressure and the cuff pressure are equal to each other. During the measurement periods Tp and Ta for measuring the pulse wave amplitude which are set before and after the pressurization period T, compliances based on the amplitudes of corrected representative values which are respectively obtained in the periods may be obtained. The obtained compliances are displayed on the displaying unit 40, independently or together with the ratio of the pulse wave amplitudes which have been described, and obtained blood pressure values. In this case, data of the measured compliances may be caused to remain as history information, the information may be formed as a table or a graph, and the trend may be displayed on the displaying unit 40.

Claims

1. An apparatus for evaluating a vascular endothelial function comprising:

a first cuff (11) which is to be wrapped around one of right and left upper or lower limbs of a subject;
a second cuff (51) which is to be wrapped around the one of the right and left upper or lower limbs, around which the first cuff (11) is to be wrapped;

a third cuff (71) which is to be wrapped around another one of the right and left upper or lower limbs, the other one limb being opposite to the one limb around which the first cuff (11) and the second cuff (51) are to be wrapped;

a cuff pressure controller (20) which controls pressures that are applied to the first cuff (11), the second cuff (51) and the third cuff (71), respectively;

a cuff pressure detector (31) which, from an output of a pressure sensor (54) connected to the second cuff (51), and an output of a pressure sensor (74) connected to the third cuff (71), detects cuff pressures in the second cuff (51) and the third cuff (71);

a pulse wave detector (32) which detects respective pulse waves at the second cuff (51) and the third cuff (71) from outputs of the pressure sensors; and

an analyzer (33) which analyzes the detected pulse waves to evaluate a vascular endothelial function,

wherein the cuff pressure controller (20) controls the cuff (11) pressure of the first cuff to avascularize the one limb around which the first cuff (11) is wrapped, for a predetermined time period,

the pulse wave detector (32) detects a pulse wave corresponding to the second cuff (51), and a pulse wave corresponding to the third cuff (71), before and after the avascularization in a state where the cuff pressures of the second (51) and third cuffs (71) are controlled to respective predetermined pressures by the cuff pressure controller (20),

the analyzer (33) corrects the pulse waves which correspond to the second cuff (51) and are detected before and after the avascularization, by the pulse waves which correspond to the third cuff (71) and are detected before and after the avascularization, and

the analyzer (33) evaluates the vascular endothelial function based on the corrected pulse waves corresponding to the second cuff (51).

2. An apparatus for evaluating a vascular endothelial function wherein the apparatus includes:

a second cuff (51) which is to be wrapped around one of right and left upper or lower limbs of a subject;

a third cuff (71) which is to be wrapped around another one of the right and left upper or lower limbs, the other one limb being opposite to the one limb around which the second cuff (51) is to be wrapped;

a cuff pressure controller (20) which controls pressures that are applied to the second cuff

- (51) and the third cuff (71), respectively;
 a cuff pressure detector (31) which, from an output of a pressure sensor (54) connected to the second cuff (51), and an output of a pressure sensor (74) connected to the third cuff (71), detects cuff pressures in the second cuff (51) and the third cuff (71);
 a pulse wave detector (32) which detects respective pulse waves at the second cuff (51) and the third cuff (71) from outputs of the pressure sensors; and
 an analyzer (33) which analyzes the detected pulse waves to evaluate a vascular endothelial function,
 wherein the cuff pressure controller (20) controls the cuff pressure of the second cuff (51) to avascularize the one limb around which the second cuff (51) is wrapped, for a predetermined time period,
 the pulse wave detector (32) detects a pulse wave corresponding to the second cuff (51), and a pulse wave corresponding to the third cuff (71), before and after the avascularization in a state where the cuff pressures of the second (51) and third cuffs (71) are controlled to respective predetermined pressures by the cuff pressure controller (20),
 the analyzer (33) corrects the pulse waves which correspond to the second cuff (51) and are detected before and after the avascularization, by the pulse waves corresponding to the third cuff (71) and detected before and after the avascularization, and
 the analyzer (33) evaluates the vascular endothelial function based on the corrected pulse waves corresponding to the second cuff (51).
3. The apparatus for evaluating a vascular endothelial function according to claim 1 or 2, wherein the pulse waves handled in the analyzer (33) are pulse wave indexes, and the pulse wave indexes are a parameter indicating a feature of a pulse wave.
 4. The apparatus for evaluating a vascular endothelial function according to claim 3, wherein the correction corrects a result of a comparison between the pulse wave indexes corresponding to the second cuff (51) and detected before and after the avascularization.
 5. The apparatus for evaluating a vascular endothelial function according to claim 4, wherein the comparison result is ratios of the pulse wave indexes of the second cuff (51) and the third cuff (71) before and after the avascularization, and the correction corrects the ratio of the pulse wave indexes corresponding to the second cuff (51) by using the ratio of the pulse wave indexes corresponding to the third cuff (71).
 6. The apparatus for evaluating a vascular endothelial function according to claim 4 or 5, wherein the comparison and the correction are performed by using values of the pulse wave indexes corresponding to the second cuff (51) or the third cuff (71), the values being obtained at a required timing, and values of the pulse wave indexes corresponding to the third cuff (71) or the second cuff (51), the values being obtained at the required timing.
 7. The apparatus for evaluating a vascular endothelial function according to claim 4 or 5, wherein the comparison and the correction are performed by using values of the pulse wave indexes corresponding to the third cuff (71), and values of the pulse wave indexes corresponding to the second cuff (51) and equal to the values of the pulse wave indexes corresponding to the third cuff (71).
 8. The apparatus for evaluating a vascular endothelial function according to any one of claims 3 to 7, wherein the pulse wave indexes are a maximum value of a pulse wave amplitude, or a mean value in the vicinity of the maximum value.
 9. The apparatus for evaluating a vascular endothelial function according to any one of claims 1 to 8, wherein the analyzer (33) further performs a process of obtaining a systolic blood pressure and a diastolic blood pressure, and dividing an amplitude of the detected pulse wave by a difference between the systolic blood pressure and the diastolic blood pressure, thereby obtaining a compliance of a blood vessel.

FIG. 1

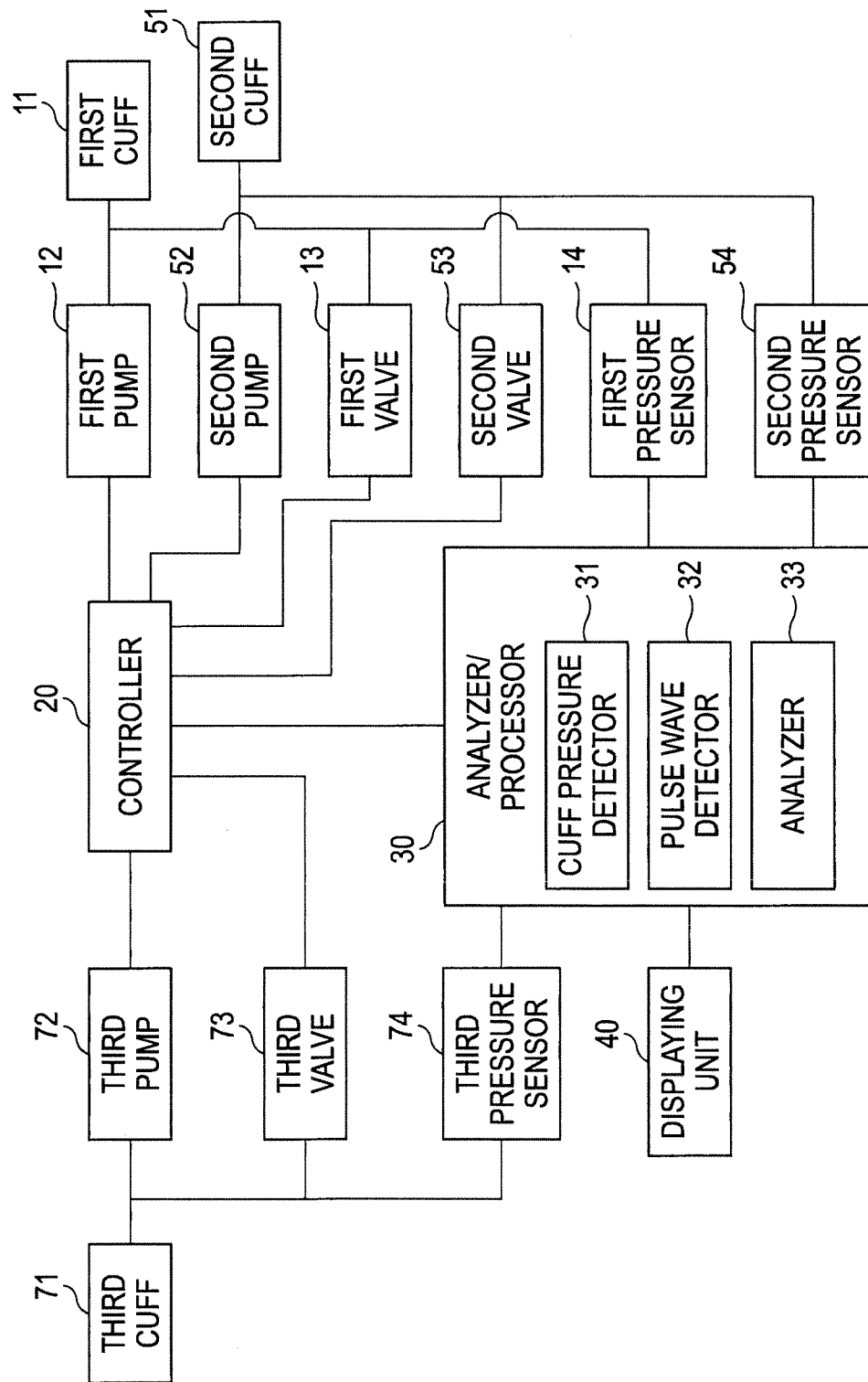


FIG. 2

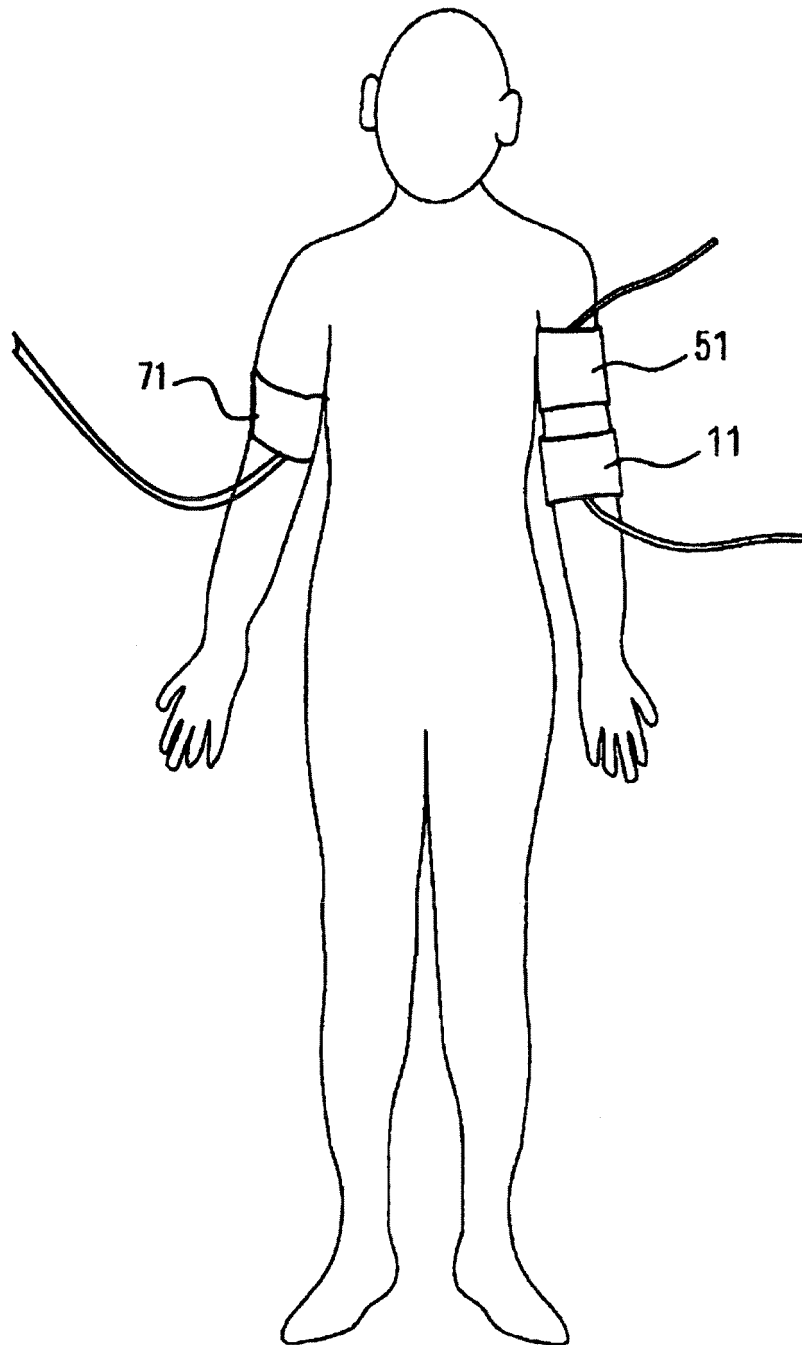


FIG. 3A

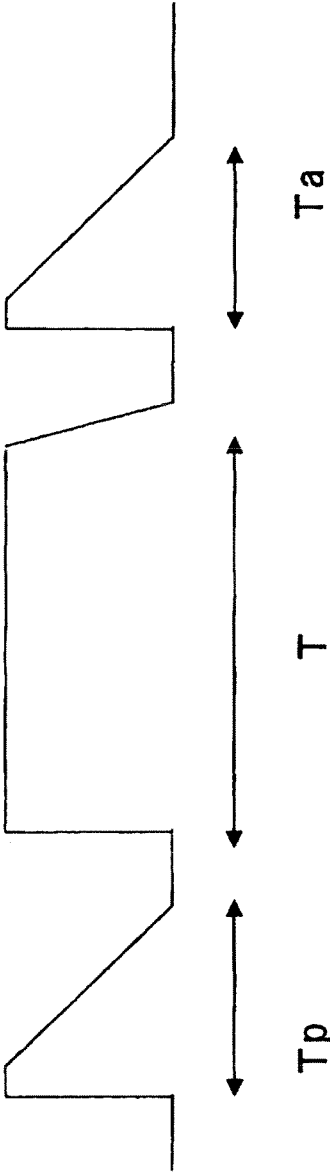


FIG. 3B



FIG. 3C



FIG. 4

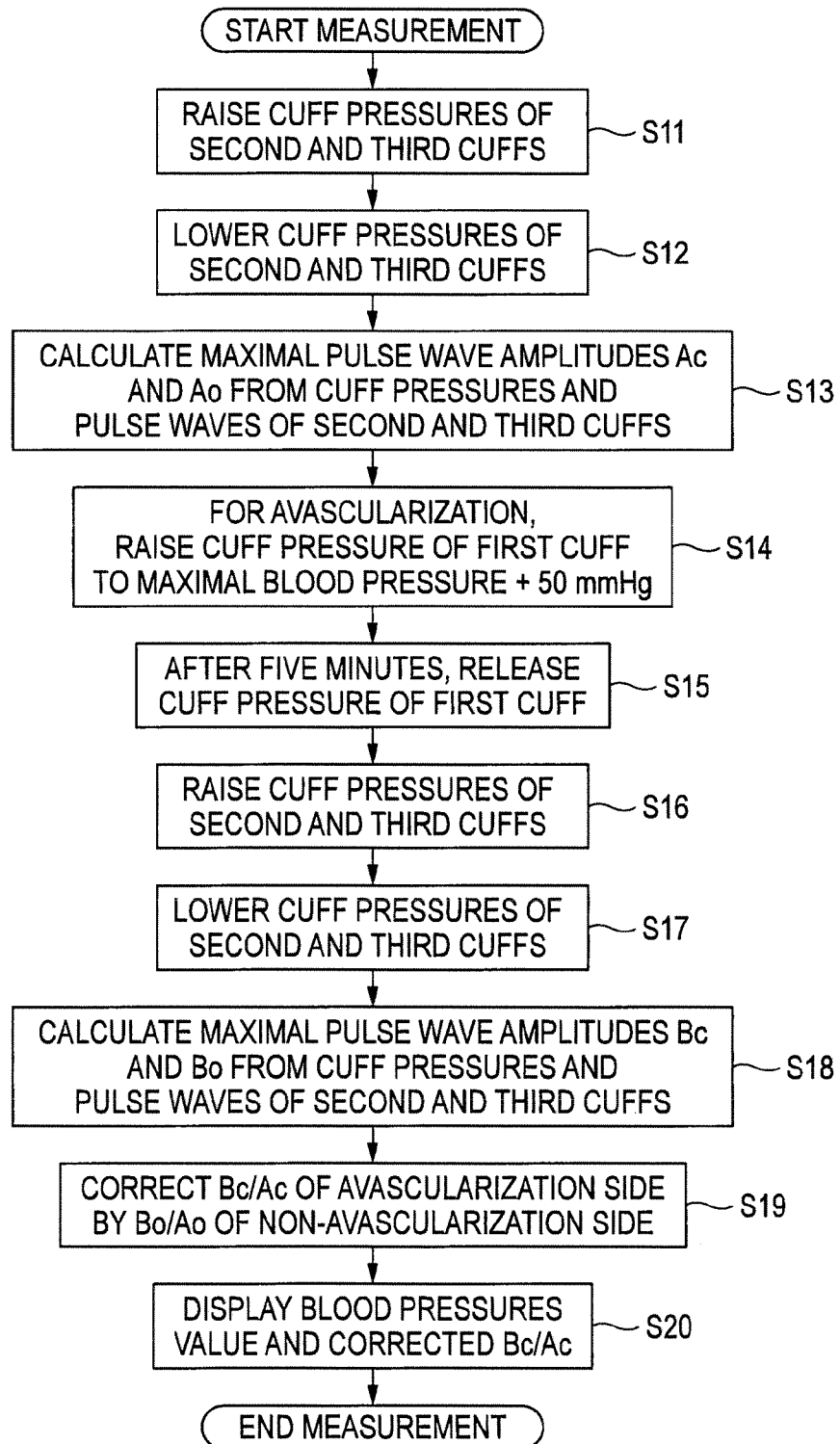


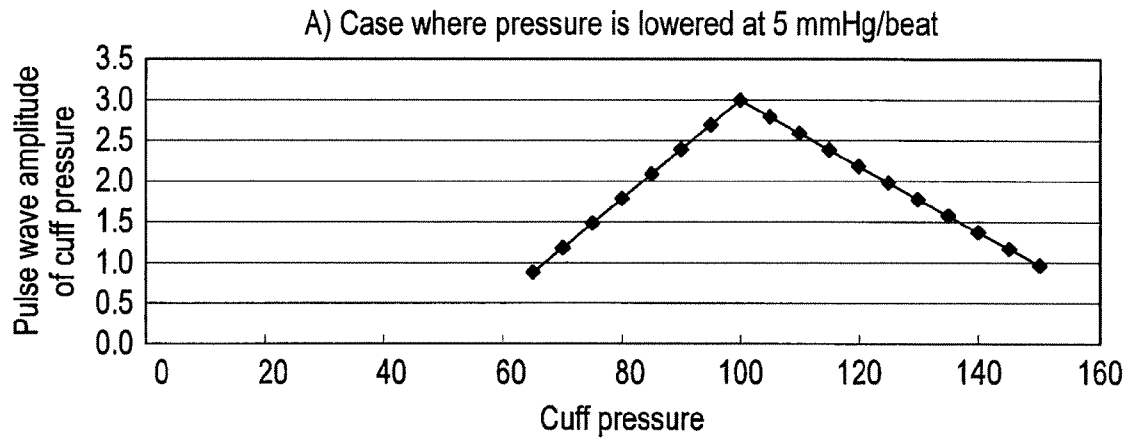
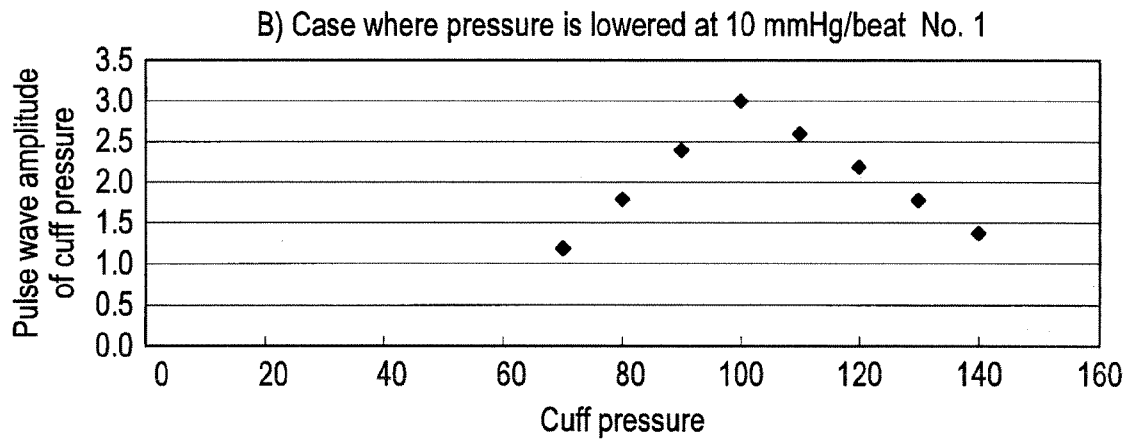
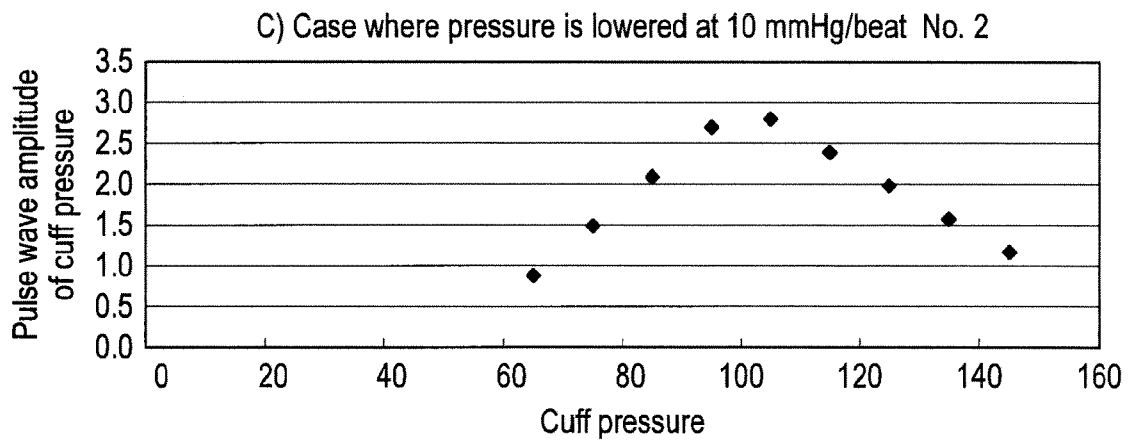
FIG. 5A**FIG. 5B****FIG. 5C**

FIG. 6A

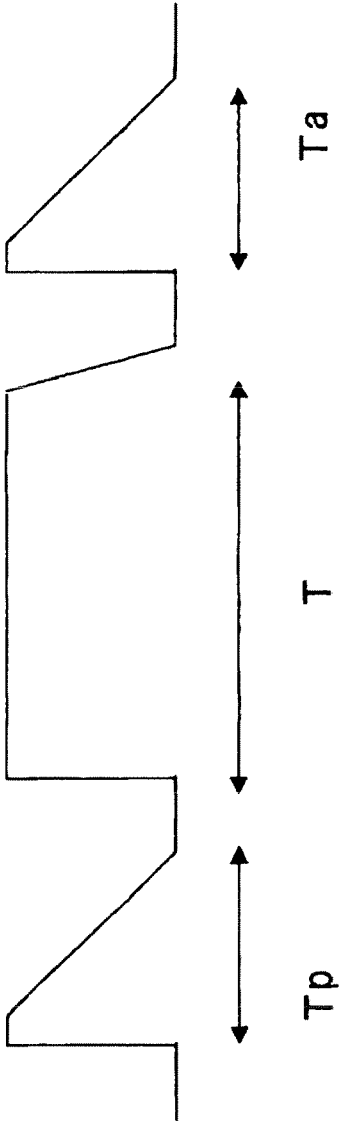


FIG. 6B

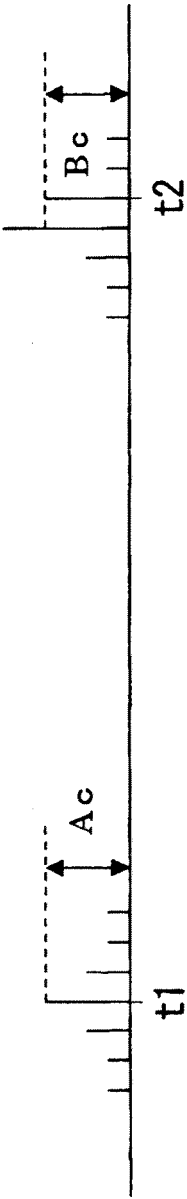


FIG. 6C

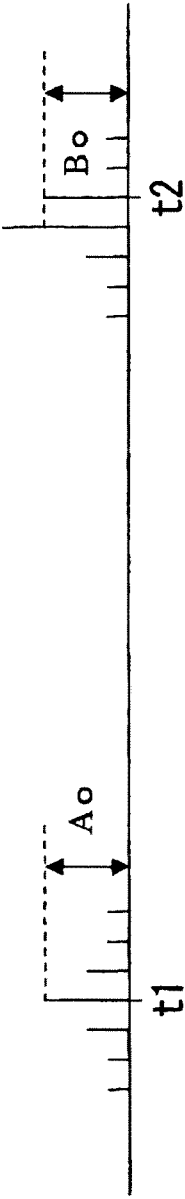


FIG. 7A

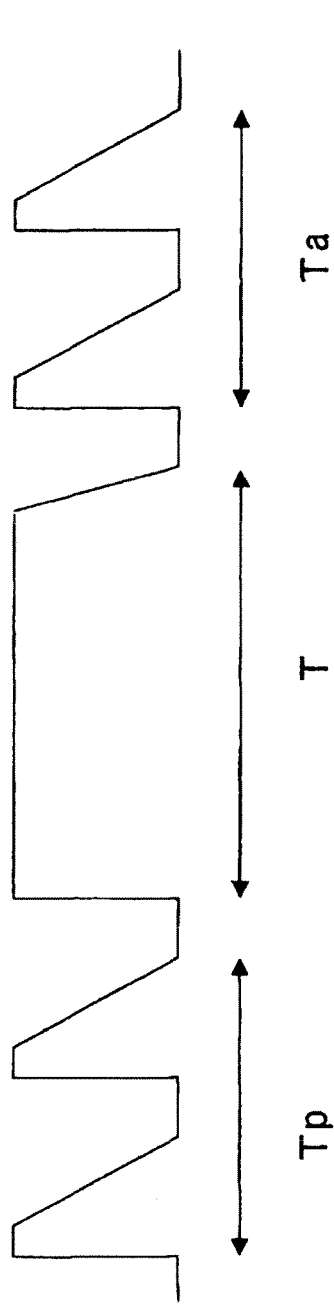


FIG. 7B

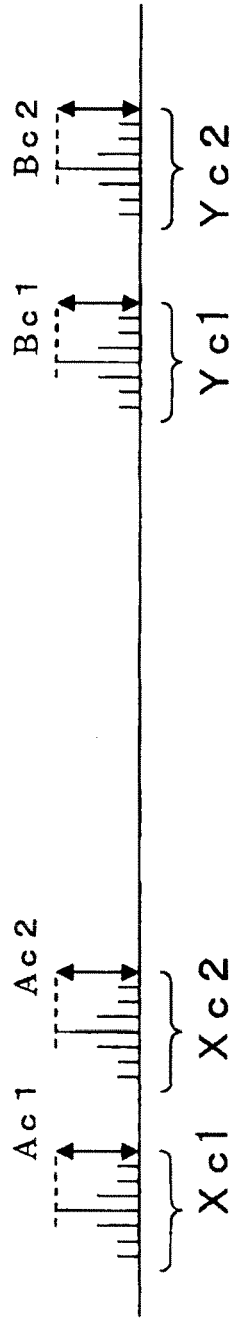
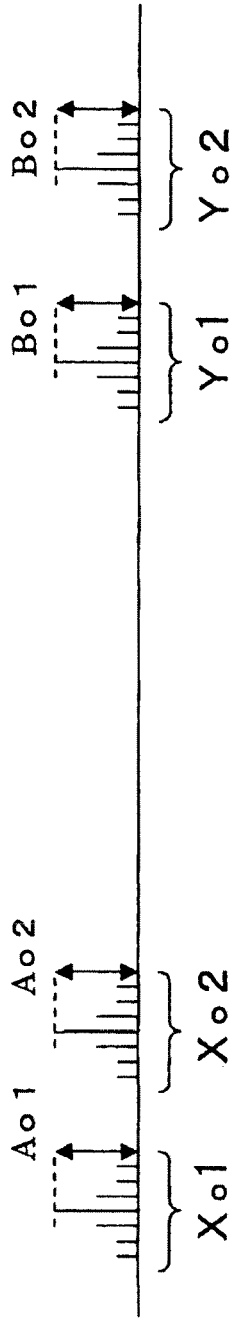


FIG. 7C



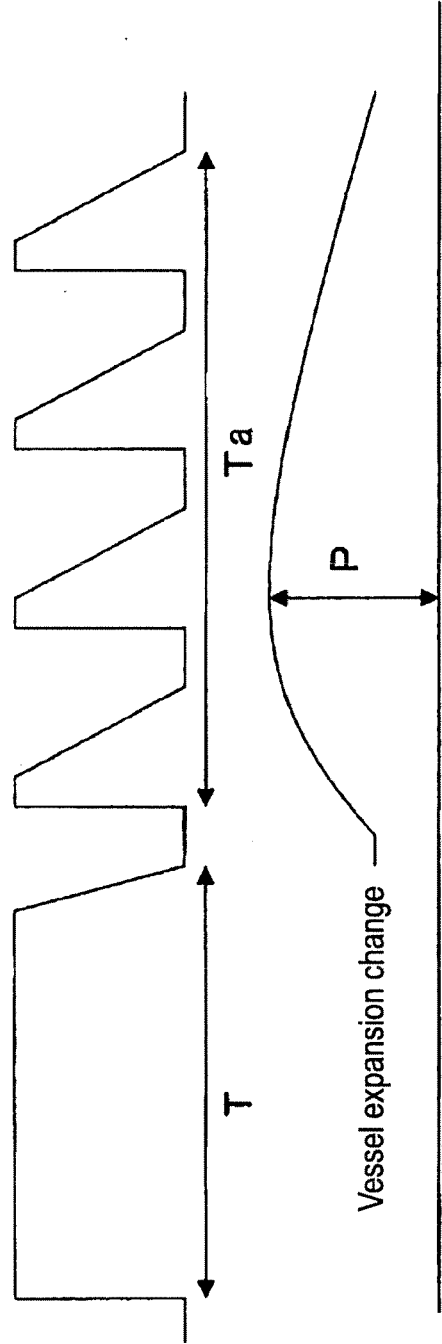


FIG. 8A

FIG. 8B



FIG. 8C

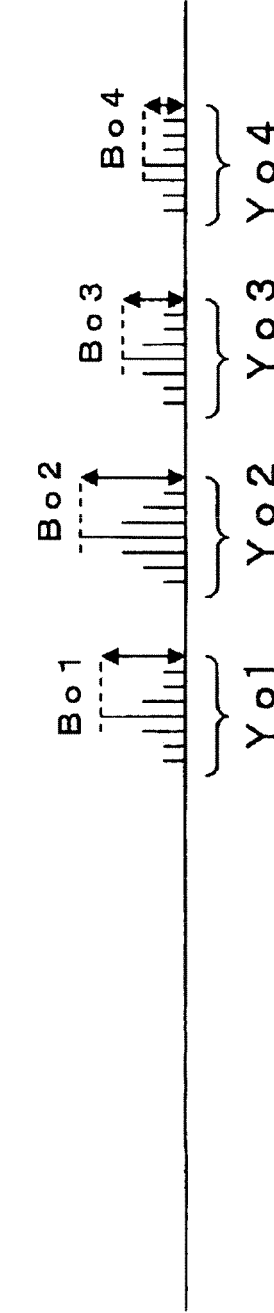


FIG. 8D



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Application Number
EP 15 15 0971

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A	EP 2 606 818 A1 (UNIV HIROSHIMA [JP]; NIHON KOHDEN CORP [JP]) 26 June 2013 (2013-06-26) * claims; figures * * paragraph [0040] - paragraph [0064] * * paragraph [0025] - paragraph [0039] *	1-9	
A	CN 202 909 061 U (WU GUIFU) 1 May 2013 (2013-05-01) * the whole document *	1-9	
A	WO 2012/149209 A1 (UNIV CALIFORNIA [US]; MALTZ JONATHAN S [US]) 1 November 2012 (2012-11-01) * the whole document *	1-9	TECHNICAL FIELDS SEARCHED (IPC) A61B
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The present search report has been drawn up for all claims			
Place of search Munich		Date of completion of the search 9 June 2015	Examiner Mundakapadam, S
CATEGORY OF CITED DOCUMENTS X : particularly relevant if taken alone Y : particularly relevant if combined with another document of the same category A : technological background O : non-written disclosure P : intermediate document T : theory or principle underlying the invention E : earlier patent document, but published on, or after the filing date D : document cited in the application L : document cited for other reasons & : member of the same patent family, corresponding document			

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专利名称(译)	评估血管内皮功能的装置		
公开(公告)号	EP2896358A1	公开(公告)日	2015-07-22
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申请(专利权)人(译)	日本光电公司		
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IPC分类号	A61B5/00 A61B5/02 A61B5/021 A61B5/022 A61B5/0235		
CPC分类号	A61B5/02007 A61B5/02028 A61B5/02108 A61B5/02116 A61B5/02141 A61B5/022 A61B5/02233 A61B5/026 A61B5/6824		
代理机构(译)	BREVALEX		
优先权	2014008465 2014-01-21 JP		
其他公开文献	EP2896358B1		
外部链接	Espacenet		

摘要(译)

一种用于评估血管内皮功能的装置，包括围绕受试者的左右上肢或下肢之一缠绕的第一箍带，围绕右上肢和左上肢或下肢之一缠绕的第二箍带，第三箍带缠绕在左右上肢或下肢中的另一个上的袖带压力控制器，其分别控制施加到第一袖带，第二袖带和第三袖带的压力，袖带压力检测器，其检测袖带压力。第二袖带和第三袖带是脉搏波检测器，其从压力传感器的输出检测第二袖带和第三袖带处的各个脉搏波。

FIG. 1

