



(11) **EP 3 227 699 B1**

(12) **EUROPEAN PATENT SPECIFICATION**

(45) Date of publication and mention
of the grant of the patent:
29.08.2018 Bulletin 2018/35

(51) Int Cl.:
G01R 33/28 ^(2006.01) **G01R 33/3415** ^(2006.01)
A61B 5/055 ^(2006.01) **A61B 5/01** ^(2006.01)
A61B 5/00 ^(2006.01)

(21) Application number: **15801856.4**

(86) International application number:
PCT/EP2015/078067

(22) Date of filing: **30.11.2015**

(87) International publication number:
WO 2016/087376 (09.06.2016 Gazette 2016/23)

(54) **MAGNETIC RESONANCE IMAGING SYSTEM WITH INFRARED THERMOMETRY SENSORS**
MAGNETRESONANZBILDGEBUNGSSYSTEM MIT INFRAROT-THERMOMETRIESENSOREN
SYSTÈME D'IMAGERIE PAR RÉSONANCE MAGNÉTIQUE AVEC CAPTEURS DE THERMOMÉTRIE
INFRAROUGE

(84) Designated Contracting States:
**AL AT BE BG CH CY CZ DE DK EE ES FI FR GB
GR HR HU IE IS IT LI LT LU LV MC MK MT NL NO
PL PT RO RS SE SI SK SM TR**

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(30) Priority: **04.12.2014 EP 14196342**

(56) References cited:
JP-A- 2008 212 437 JP-A- 2009 183 472

(43) Date of publication of application:
11.10.2017 Bulletin 2017/41

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- **IBRAHIM T SET AL: "Evaluation of MRI RF probes
utilizing infrared sensors", IEEE
TRANSACTIONS ON BIOMEDICAL
ENGINEERING IEEE USA, vol. 53, no. 5, May 2006
(2006-05), pages 963-967, XP002740462, ISSN:
0018-9294**

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Description

TECHNICAL FIELD OF THE INVENTION

[0001] The invention relates to magnetic resonance imaging, in particular to apparatus and methods for preventing the overheating of a subject during magnetic resonance imaging.

BACKGROUND OF THE INVENTION

[0002] A static magnetic field is used by Magnetic Resonance Imaging (MRI) scanners to align the nuclear spins of atoms as part of the procedure for producing images within the body of a patient. This static magnetic field is referred to as the B_0 field. It is commonly known that increasing the strength of the B_0 field used for performing an MRI scan offers the opportunity of increasing the spatial resolution and contrast resolution of the diagnostics images. This increase in resolution and contrast benefits physicians using an MRI image to diagnose a patient.

[0003] During an MRI scan, Radio Frequency (RF) pulses generated by a transmitter coil cause perturbations to the local magnetic field. These perturbations are known as the B_1 field. The B_1 field is used to manipulate the orientation of the nuclear spins. These RF signals are used to construct the MRI images. These coils can also be referred to as antennas. Further, the transmitter and receiver coils can also be integrated into a single transceiver coil that performs both functions. It is understood that the use of the term transceiver coil also refers to systems where separate transmitter and receiver coils are used. A difficulty is that the B_1 field can also cause heating of the subject being imaged. To image regions deep within the body of a subject, the surface regions of the subject can be exposed to levels of radiation which can overheat tissue. The term Specific Absorption Ratio (SAR) is the radio frequency power absorbed per unit mass in tissue and is a measure of this overheating.

[0004] European patent application EP0 841 576 discloses a probe designed to be inserted into and removed from a patient that carries at least one sensor used for control the target of energy related to an interventional procedure. In the Japanese patent application JP2008-212437 an RF transmission coil with a decoupling circuit is disclosed. The decoupling circuit is provided with a temperature sensor. The high-frequency irradiation is stopped when the temperature exceeds a predetermined threshold.

[0005] The decoupling circuit is provided with a temperature sensor. The high-frequency irradiation is stopped when the temperature exceeds a predetermined threshold.

SUMMARY OF THE INVENTION

[0006] The invention relates to a magnetic resonance

imaging system, a method of operating a magnetic resonance imaging system and a magnetic resonance imaging antenna in independent claims. Embodiments are given in the dependent claims.

[0007] In one aspect the invention provides for a magnetic resonance imaging system according to claim 9. The magnetic resonance imaging system comprises a magnetic resonance imaging antenna comprising multiple loop antenna elements. The magnetic resonance imaging antenna further comprises multiple infrared thermometry sensors. Notably, an individual infrared thermometry sensors may be associated with one of the antenna elements; such an antenna element is formed as a conductor loop for transmitting a radio frequency field or for receiving radio frequency magnetic resonance signals. For example, each infrared thermometry sensor may be associated with one of the antenna loops. An infrared thermometry sensor as used herein encompasses a sensor which can measure temperature by using infrared radiation. The magnetic resonance imaging antenna is configured for being positioned adjacent to an external surface of the subject. At least a portion of the multiple infrared thermometry sensors are directed towards the external surfaces when the magnetic resonance imaging antenna is positioned adjacent to the external surface of the subject. An alternative way of wording this is that the magnetic resonance imaging antenna has an outer surface and that the multiple infrared thermometry sensors are able to measure the surface temperature of objects adjacent to the outer surface.

[0008] The magnetic resonance imaging system further comprises a memory containing machine executable instructions and pulse sequence instructions. Pulse sequence instructions as used herein encompass commands or a sequence of events such as events in a timeline which can be converted into commands; they may be used to control the magnetic resonance imaging system to acquire the magnetic resonance data according to a magnetic resonance imaging technique. The magnetic resonance imaging system further comprises a processor for controlling the magnetic resonance imaging system. Execution of the machine executable instructions causes the processor to acquire the magnetic resonance data by controlling the magnetic resonance imaging system with the pulse sequence instructions. Execution of machine executable instructions further causes the processor to repeatedly measure at least one surface temperature of the subject with the multiple infrared thermometry sensors during acquisition of the magnetic resonance data. Alternatively this may be worded in that the machine executable instructions cause the processor to repeatedly measure at least one temperature with the multiple infrared thermometry sensors during acquisition of the magnetic resonance data. Execution of the machine executable instructions further causes the processor to perform a predefined action if at least one surface temperature is above a predefined surface temperature. If at least one of the multiple infrared thermometry sen-

sors measures a temperature which is above the predefined temperature then the processor takes a specific or predefined action. This example may have the benefit that the magnetic resonance imaging system can react automatically to heating caused by the acquisition of magnetic resonance data. That is the action taken by the processor achieves to reduce the risk of the subject becoming overheated.

[0009] In another example the antenna could be a transmit and/or a receive antenna. That is to say the antenna may be in some instances used for receiving magnetic resonance data and in other instances may be used for transmitting radio frequency pulses for manipulating spins of the subject within the imaging zone.

[0010] In another embodiment each of the multiple loop antennas have current leads. A current lead as used herein is a point on the antenna where radio frequency current is fed into or received from the multiple loop antenna element. At least a subset of the multiple infrared thermometry sensors is positioned in an offset region. The current leads are within the offset region. The offset region may alternatively be defined or described as a region of each of the multiple loop antennas which is near or adjacent to the current leads. That is, the offset region is located offset from the geometrical centre of the conductor (coil) loop of the individual antenna element. It may be beneficial to place the multiple infrared thermometry sensors at the position for the current leads because the voltage or the area with the largest electric fields may be near the location of the current leads. If the antenna is a transmit antenna it may be expected that the heating of the subject by the magnetic resonance imaging antenna would be near to the regions where the current leads are.

[0011] In another embodiment each of the multiple loop antennas have current leads. The current leads as used herein are commonly interrupted by capacitors. At least a subset of the multiple infrared thermometry sensors is positioned next to the current leads. It may be beneficial to place the multiple infrared thermometry sensors at the position of the capacitors because the voltage or the area with the largest electric fields may alternatively be near the location of the capacitors. If the antenna is a transmit antenna it may be expected that the heating of the subject by the magnetic resonance imaging antenna would be near to the regions where the capacitors are.

[0012] In another embodiment the magnetic resonance imaging antenna is configured for functioning as a transmit antenna. For example, the magnetic resonance imaging antenna may be connected to a transmitter or a transceiver. The magnetic resonance imaging system comprises a radio frequency system for supplying radio frequency power to each of the subset of multiple antenna elements. The predefined action comprises reducing the radio frequency power supplied to an antenna element if an infrared thermometry sensor in the offset region of the loop antenna element measures a surface temperature above the predefined temperature. The in-

frared thermometry sensor is chosen from the subset of the multiple infrared thermometry sensors. The loop antenna element is chosen from the subset of multiple antenna elements. In this example, the surface temperature is measured adjacent to a particular loop antenna element. If the surface temperature of the subject is above the threshold then the radio frequency system can automatically reduce the power supplied to that particular loop antenna element thus reducing the heating of the subject.

[0013] In some examples the RF power is reduced by either changing a flip angle of the imaging sequence which is in the full sequence instructions or by relaxing or pausing the time regime of the pulse sequence.

[0014] In another embodiment, at least a portion of the multiple infrared thermometry sensors are each positioned in a central region of a loop antenna element chosen from the multiple loop antenna elements.

[0015] The multiple infrared thermometry sensors positioned in the central region may be used in the same way as the infrared thermometry sensors, which are positioned in an offset region that is next to the current leads and/or capacitors. For example if the loop antenna element measures too high of a surface temperature this may then also cause the radio frequency system to reduce the power supplied to the loop antenna element which the infrared thermometry sensor is closest to.

[0016] In another embodiment the magnetic resonance imaging antenna is configured for functioning as a receive antenna. For example the magnetic resonance imaging antenna may be connected to a receiver or a transceiver.

[0017] In another embodiment the magnetic resonance imaging antenna comprises a subject support configured for supporting the subject on a support surface at least partially within the imaging zone. At least a portion of the antenna elements are arranged within the subject support and adjacent to the support surface. In this example at least a part of the magnetic resonance imaging antenna is built into the subject support. Incorporating the antenna elements with the infrared thermometry sensors into the subject support may have the benefit that it reduces the chances of the subject being overheated during the acquisition of magnetic resonance data.

[0018] In another embodiment the magnetic resonance imaging antenna comprises a flexible surface antenna. The flexible surface antenna is configured for being placed in contact with a portion of outer surface of the subject. In this example at least a part of the magnetic resonance imaging antenna is a flexible antenna which can be placed over or about the subject. The use of the infrared thermometry sensors may be beneficial because it is difficult to have direct contact with the antenna and the subject. Using the infrared thermometry sensors enables the antenna to be used and accurately measure the temperature of the subject without being in physical contact.

[0019] In another embodiment the magnetic resonance imaging system comprises an air cooling system

for cooling the subject within the imaging zone with an airflow. The predefined action comprises increasing airflow if the surface temperature is above the predefined temperature.

[0020] In another embodiment execution of the machine executable instructions further causes the processor to select the predefined temperature from a table of predefined temperatures using any one of the following criterion or criteria: subject weight, subject age, subject type, subject size, and combinations of thereof.

[0021] The use of such a criterion may be useful because models can be developed using empirical data or modeled information.

[0022] In another embodiment the predefined action is the halting of the acquisition of the magnetic resonance data. In this embodiment the predefined action is to break off the acquisition of magnetic resonance data

[0023] In another embodiment the predefined action is the modification of the pulse sequence instructions. This for instance may cause a particular loop antenna element to have its power reduced, the particular phase or flip angle sent to it, or even pauses during the acquisition of the magnetic resonance data. That, the pausing means that acquisition of magnetic resonance data is interrupted temporarily, until the surface temperature may fall below the predefined temperature, or even below a safety margin below the predefined temperature.

[0024] In another embodiment the predefined action is the increase of the air ventilation to a subject to increase cooling.

[0025] In another embodiment the predefined action is the pausing or delaying of the acquisition of the magnetic resonance data.

[0026] In accordance with claim 6, the invention provides for a method of operating a magnetic resonance imaging system requiring magnetic resonance data from a subject within an imaging zone period. The magnetic resonance imaging system comprises a magnetic resonance imaging antenna comprising multiple antenna elements. Each of the antenna elements is a loop antenna element. The magnetic resonance imaging antenna further comprises multiple infrared thermometry sensors. The magnetic resonance imaging antenna is configured for being positioned adjacent to an external surface of the subject. At least a portion of the multiple infrared thermometry sensors are directed towards the external surface when the magnetic resonance imaging antenna is positioned adjacent to the external surface. The method comprises the steps of acquiring the magnetic resonance data by controlling the magnetic resonance imaging system with pulse sequence instructions. The method further comprises the step of repeatedly measuring a surface temperature of the subject with each of the multiple infrared thermometry sensors during acquisition of the magnetic resonance data. The method comprises of performing a predefined action if the surface temperature is above a predefined temperature.

[0027] In another embodiment, the method further

comprises placing an infrared transparent garment on the outer surface on the subject before acquiring the magnetic resonance data. This may be beneficial because the infrared sensors are used to measure the surface temperature of the subject. If the subject is wearing a normal garment then the fabric or material of the garment may block the measurement of the surface temperature of the subject. Using an infrared transparent garment or one with a high infrared transparent transmissivity may enable the measurement to be made even if the subject is wearing a garment.

[0028] In another embodiment, the infrared transparent garment is fabricated at least partially from polyethylene foil. The use of polyethylene foil to manufacture the infrared transparent garment may be beneficial because polyethylene foil has a high degree of transmission of infrared light. The invention also provides for a magnetic resonance imaging antenna comprising multiple antenna elements, as defined in claim 1. Each of the antenna elements is a loop antenna element. The magnetic resonance imaging antenna further comprises multiple infrared thermometry sensors. The magnetic resonance imaging antenna is configured for being positioned adjacent to an external surface of the subject. At least a portion of the multiple infrared thermometry sensors are directed towards the external surface when the magnetic resonance imaging antenna is positioned adjacent to the external surface, for measuring a surface temperature of the subject with the multiple infrared thermometry sensors. In another embodiment the magnetic resonance imaging antenna is integrated into a subject support.

[0029] It is understood that one or more of the aforementioned embodiments of the invention may be combined as long as the combined embodiments are not mutually exclusive.

BRIEF DESCRIPTION OF THE DRAWINGS

[0030] In the following preferred embodiments of the invention will be described, by way of example only, and with reference to the drawings in which:

Fig. 1 illustrates an example of a magnetic resonance imaging system;

Fig. 2 shows a flow chart that illustrates a method of operating the magnetic resonance imaging system of Fig. 1;

Fig. 3 illustrates a further example of a magnetic resonance imaging system;

Fig. 4 shows an enlarged view of a portion of Fig. 3;

Fig. 5 illustrates an example of a magnetic resonance imaging antenna;

Fig. 6 illustrates a further example of a magnetic resonance imaging antenna;

Fig. 7 illustrates a further example of a magnetic resonance imaging antenna; and

Fig. 8 illustrates a further example of a magnetic resonance imaging antenna.

DETAILED DESCRIPTION OF THE EMBODIMENTS

[0031] Like numbered elements in these figures are either equivalent elements or perform the same function. Elements which have been discussed previously will not necessarily be discussed in later figures if the function is equivalent.

[0032] Fig. 1 shows an example of a magnetic resonance imaging system 100 with a magnet 104. The magnet 104 is a superconducting cylindrical type magnet 104 with a bore 106 through it. The use of different types of magnets is also possible; for instance it is also possible to use both a split cylindrical magnet and a so called open magnet. A split cylindrical magnet is similar to a standard cylindrical magnet, except that the cryostat has been split into two sections to allow access to the iso-plane of the magnet, such magnets may for instance be used in conjunction with charged particle beam therapy. An open magnet has two magnet sections, one above the other with a space in-between that is large enough to receive a subject: the arrangement of the two sections area similar to that of a Helmholtz coil. Open magnets are popular, because the subject is less confined. Inside the cryostat of the cylindrical magnet there is a collection of superconducting coils. Within the bore 106 of the cylindrical magnet 104 there is an imaging zone 108 where the magnetic field is strong and uniform enough to perform magnetic resonance imaging.

[0033] Within the bore 106 of the magnet there is also a set of magnetic field gradient coils 110 which is used for acquisition of magnetic resonance data to spatially encode magnetic spins within the imaging zone 108 of the magnet 104. The magnetic field gradient coils 110 connected to a magnetic field gradient coil power supply 112. The magnetic field gradient coils 110 are intended to be representative. Typically magnetic field gradient coils 110 contain three separate sets of coils for spatially encoding in three orthogonal spatial directions. A magnetic field gradient power supply supplies current to the magnetic field gradient coils. The current supplied to the magnetic field gradient coils 110 is controlled as a function of time and may be ramped or pulsed.

[0034] Adjacent to the imaging zone 108 is a magnetic resonance antenna 113 for manipulating the orientations of magnetic spins within the imaging zone 108 and for receiving radio transmissions from spins also within the imaging zone 108. The radio frequency antenna contain multiple coil elements 114. The radio frequency antenna may also be referred to as a channel or antenna. The magnetic resonance antenna 113 is connected to a radio frequency transceiver 116. The magnetic resonance antenna 113 and radio frequency transceiver 116 may be replaced by separate transmit and receive coils and a separate transmitter and receiver. It is understood that the magnetic resonance antenna 113 and the radio frequency transceiver 116 are representative. The magnetic resonance antenna 113 may also represent a dedicated transmit antenna and a dedicated receive antenna.

Likewise the transceiver 116 may also represent a separate transmitter and receivers. The magnetic resonance antenna 113 may also have multiple receive/transmit elements and the radio frequency transceiver 116 may have multiple receive/transmit channels. The transmit antenna may also be built into the bore of the magnet in a layer beneath (more central) to the gradient coil.

[0035] The subject support 120 is attached to an optional actuator 122 that is able to move the subject support and the subject 118 through the imaging zone 108. The transceiver 116, the magnetic field gradient coil power supply 112 and the actuator 122 are all see as being connected to a hardware interface 128 of computer system 126.

[0036] The subject 118 can be seen as having a magnetic resonance antenna 113 placed on an outer surface 119 of the subject 118. The magnetic resonance imaging antenna 113 is made up of a number of loop antenna elements 114. Also shown is an infrared thermometry sensor 115 that is associated with each of the loop antenna elements 114. These infrared thermometry sensors 115 may be used to measure a surface temperature on the outer surface 119.

[0037] The computer storage 134 is shown as containing pulse sequence instructions 140 for performing a magnetic resonance fingerprinting technique. The computer storage 134 is further shown as containing magnetic resonance data 142 that was acquired using the pulse sequence instructions 140 to control the magnetic resonance imaging system 100. The computer storage 134 is further shown as containing a magnetic resonance image 144 that was reconstructed using the magnetic resonance data 142. The computer storage 134 is further shown as containing thermometry data 146 as measured using the infrared thermometry sensors 115. The computer storage 134 is further shown as containing a predefined temperature or a temperature model which returns a predefined temperature 148. The predefined temperature for example 148 may be used to compare against the thermometry data 146 to determine if the outer surface 119 of the subject 118 is too hot or warm.

[0038] The computer memory 136 contains a control module 150 which contains such code as operating system or other instructions which enables the processor 130 to control the operation and function of the magnetic resonance imaging system 100.

[0039] The computer memory 136 is further shown as containing an image reconstruction module 152 that uses the magnetic resonance data 142 to reconstruct the magnetic resonance image 144.

[0040] Fig. 2 shows a flow chart which illustrates a method of operating the magnetic resonance imaging system 100 of Fig. 1. First in step 200, the magnetic resonance data 142 is acquired by controlling the magnetic resonance imaging system 100 with the pulse sequence instructions 142. Next in step 202, the processor 130 measures at least one surface temperature with the infrared thermometry sensors 115. This is stored as ther-

metry data 146 in the computer storage 134. The next step is a decision box with the question: is a measured surface temperature above the predefined temperature? If yes, then the method proceeds to step 204. If no, then the method proceeds to step 206. In step 204, the processor 130 performs a predefined action if the thermometry data 146 or at least one surface temperature is above a predefined temperature 148. Step 206 is another decision box. The question for box 206 is: Is the acquisition of magnetic resonance data finished. If yes, the method proceeds to step 208. In step 208 the method ends. If the answer to the question of box 206 is no, then the method returns to step 202 where the at least one surface temperature is measured with the infrared thermometry sensors again.

[0041] Fig. 3 illustrates a further example of a magnetic resonance imaging system 300. The magnetic resonance imaging system 300 is similar to that shown in Fig. 1 with the addition of several additional features. In this example additional magnetic resonance imaging antenna 113' embedded in the subject support 120. The subject support has a support surface 302 and there are a number of loop antenna elements 114' adjacent to the supporting surface 302. There are also a number of infrared thermometry sensors 115' which are exposed to the underside of the subject 118. This enables a further measuring of the surface temperature on the outer surface 119 of the subject 118.

[0042] Fig. 4 shows an enlarged view 400 of the imaging zone 108 shown in Fig. 3. In this example there is an infrared transparent garment 402 between the infrared thermometry sensors 115, 115' and the outer surface 119 of the subject 118. The infrared transparent garment 402 enables the sensors 115, 115' to still take temperature measurements of the outer surface 119 of the subject 118. For example each of the infrared thermometry sensors 115, 115' has a line labeled 404 which shows where the sensor 115, 115' is aimed at a measurement point 406 on the surface 119 of the subject 118. It can be seen how using a large number of these sensors enables a large number of measurement points 406 where the thermometry data 146 can be acquired. It can also be seen how both magnetic resonance imaging antennas 113 and 113' do not conform to the outer surface 119 of the subject 118. However because infrared thermometry sensors 115, 115' are used it is still possible to make accurate temperature measurements at the measurement points 406.

[0043] Fig. 5 shows an alternative view of the subject 118 reposing on the subject support 120 with the magnetic resonance antenna 113 draped over the subject 118.

[0044] Fig. 6 shows an alternative way of laying out the antenna elements 114 and infrared thermometry sensors 115. In this example each of the loop antenna elements 114 has a set of current leads 600 which may be either used for either supplying RF current to the loop antenna 114 or for receiving a radio frequency signal

from the loop antenna elements 114. Each loop antenna element 114 has a central region 602 where the infrared thermometry sensor 115 is placed. Variations of the design shown in Fig. 6 may also be made. For example it is very common for the loop antenna elements 114 to be partially overlapping.

[0045] Fig. 7 shows a further modification of the design shown in Fig. 6. In this example the infrared thermometry sensors 115 are placed within an offset region 700. The offset region 700 is away from the central region and encompasses the region which contains the current leads 600. When an RF voltage or a current is applied to the current lead 600 there may be a larger electric field in that vicinity. It may therefore be beneficial for a transmit antenna to place infrared thermometry sensors 115 in this offset region 700.

[0046] Fig. 8 shows a further modification of the design shown in Fig. 7. In this example the antenna elements 114 also have capacitors 800. The offset region 700 in this example is positioned near the capacitors. The infrared thermometry sensors 115 are again placed within the offset region 700. The offset region 700 is away from the central region and encompasses the region which contains the capacitors 800. Shown in the figure are two capacitors per antenna element 114. There is an offset region 700 near each capacitor and a infrared thermometry sensor 115 in each of the offset regions 700. The example in Figs. 7 and 8 are intended to provide an example. The positioning of the current leads and any reactive components such as capacitors will vary depending upon the design of the magnetic resonance antenna. The infrared thermometry sensors 115 can be placed near portions of the antenna elements where larger heating of the subject is to be expected.

[0047] The trend towards higher field strength, shorter scan times, and the upcoming trend towards surface transmit coil arrays has increased the risk of local SAR hotspots in superficial tissue. Examples may integrate multiple Infra Red (IR) thermometers into MR surface (receive or transmit/receive) coil arrays and to monitor the surface temperature during scanning at multiple points.

[0048] The SAR model / simulations may be used to optimize the sequences while keeping SAR values in allowable limits. Such models and simulations may for example be updated such as to match or fit with the actual temperature measurements.

[0049] In case of unacceptable MRI-induced heating several countermeasures or predetermined actions may be performed:

- The MR sequence is modified to provide reduced overall SAR
- Air ventilation is increased
- Local SAR is reduced by adjusting transmit powers for individual coil elements of the transmit coil

[0050] As mentioned above, the trend towards higher

field strength, shorter scan times, and the upcoming trend towards surface transmit coils has increased the risk of local SAR hotspots in superficial tissue. SAR becomes frequently the limitation for even faster image acquisition. SAR management has been introduced to address this fact using B_1 measurements, SAR and temperature simulations and B_1 shimming to keep local SAR below allowable limits.

[0051] SAR often represents the limiting factor for faster exams. Multi-element system body coils and surface transmission coils are subject of research with the aim to increase the degrees of freedom for SAR management via B_1 shimming, but such coils are also prone to causing superficial SAR that is not easy to predict per simulation.

[0052] Measuring B_1 and SAR via temperature mapping as preparation steps for the planned exam are causing considerable increase of exam times. This problem would become even larger for multi-element transmit coils covering a large fraction of the patient, because scan times would become extremely large.

[0053] Simulation of SAR and temperature are computationally intense and require additional scans to provide a patient-specific model (including anatomy, electrical properties, and thermal properties). In addition, simulations are associated with error margins.

[0054] The SAR limits for clinical scanning themselves include safety margins because of the imperfections in SAR monitoring, and SAR models of the MR systems also include safety margins for the same reason. Such margins limit exam times more than actually required. A better knowledge of actual temperatures during scanning may allow lowering those margins.

[0055] Examples may integrate infrared thermometry sensors or multiple IR thermometers into MR surface (receive or transmit/receive) coil such that they look onto the patient such as is shown in Fig. 4. IR sensors are available in dimensions of 1-2cm that allow integration into standard coil arrays. Sensors with a cost price of about 5 USD are available that allow integration of multiple sensors e.g. on a grid pattern of 10cm spacing without increasing the cost price of the coil considerably.

[0056] IR sensors are used to maintain a smooth workflow of the examination. This would not be possible with contact temperature sensors which would need to be fixated on the skin to achieve a stable thermal contact. The IR radiation emitted by the human skin in the suitably detectable range (2-20 μm) originates not only directly from the surface of the skin but also from a layer of superficial tissue of about 1mm, hence effectively the temperature of that layer is measured.

[0057] Special IR transparent clothes for the patient may also be fabricated, which are mostly IR transparent in the range of the detected radiation.

[0058] The main components of IR pyrometer are non-conductive and non-ferromagnetic: IR window, IR lens, thermocouple sensor with wires (made from e.g. copper, constantan, chromel, nicrosil, nisl, Rhodium, Platinum, PtRh). Devices with plastic housings are available (see

below). It is possible to use thermocouples equipped with shielded wires to measure MRI-induced heating. Connective wires have to be shielded and probably equipped with common-mode current traps as it is state-of-the-art in wiring of the MR receive elements themselves.

[0059] The temperature is expected to rise after application of the surface coil and introduction of the patient into the bore. However, this temperature should relatively quickly approach a steady state. Residual baseline drifts that are present short before scanning are determined and corrected. MRI-induced temperature increases may be monitored in real-time during scanning and temperature data is fed into the MR host computer.

[0060] In general, any simulations that have been performed before the scan as part of the SAR model that is used to optimize the sequence are updated such as to comply with the actual temperature. If the grid of temperature readings across the patient is sufficiently dense, the absence of relevant MR induced heating may be used to recalculate the current and subsequent sequences to shorten the acquisition time.

[0061] In case of unacceptable MRI-induced heating several countermeasures can be performed, initiated and controlled by the MR host computer:

- The MR sequence is modified to provide reduced overall SAR
- Air ventilation is increased
- Local SAR is reduced by adjusting transmit powers for individual coil elements of the transmit coil.

[0062] Advances in electronic and detector technology have resulted in a variety of non-contact IR thermometers for industrial and scientific use. IR detectors fall into two main groups: quantum detectors and thermal detectors (pyrometers). Quantum detectors are semiconductors that interact directly with the impacting photons, resulting in electron pairs and therefore an electrical signal. Thermal detectors change their temperature depending upon the impacting radiation which is then detected mostly by a thermocouple.

[0063] Since only single point measurements are required in this invention and response times are below 0.1 s pyrometers can be used which typically detect the IR spectrum in the range of 2-20 μm . They are available pre-calibrated for a certain temperature range (e.g. $37 \pm 5^\circ \text{C}$) and emissivity (i.e. 0.95 as for human skin). These instruments provide an absolute accuracy of better than 0.5°C in the 10°C range. The precision, i.e., the repeatability error for measurements under identical conditions is extraordinarily small, typically in the range of 0.01°C . Temporal response is better than 10 Hz.

[0064] The absolute reading of a simple pyrometer is only correct if the emissivity of the inspected surface is known and the pyrometer is calibrated for this emissivity. The emissivity of human skin is about 0.95 as for most organic substances and does not vary appreciably with wavelength. Common IR detectors pre-calibrated for

0.95 are available.

IR transparency of clothes

[0065] Clothes are commonly made from polymers some of which are already relative IR transparent in the required range. However, especially polyethylene (C₂H₄)_n is highly transparent to IR with only three narrow absorption maxima in the range of 2-20 μm. It is less commonly used for standard clothes. Still, it is proposed to design patient clothes preferably made from polyethylene, potentially with some polyamide or polyester fiber content. An example of such clothes are labeled 402 in Fig. 4.

[0066] While the invention has been illustrated and described in detail in the drawings and foregoing description, such illustration and description are to be considered illustrative or exemplary and not restrictive; the invention is not limited to the disclosed embodiments.

[0067] Other variations to the disclosed embodiments can be understood and effected by those skilled in the art in practicing the claimed invention, from a study of the drawings, the disclosure, and the appended claims. In the claims, the word "comprising" does not exclude other elements or steps, and the indefinite article "a" or "an" does not exclude a plurality. A single processor or other unit may fulfill the functions of several items recited in the claims. The mere fact that certain measures are recited in mutually different dependent claims does not indicate that a combination of these measures cannot be used to advantage. A computer program may be stored/distributed on a suitable medium, such as an optical storage medium or a solid-state medium supplied together with or as part of other hardware, but may also be distributed in other forms, such as via the Internet or other wired or wireless telecommunication systems. Any reference signs in the claims should not be construed as limiting the scope.

LIST OF REFERENCE NUMERALS

[0068]

100 magnetic resonance system
104 magnet
106 bore of magnet
108 measurement zone or imaging zone
110 magnetic field gradient coils
112 magnetic field gradient coil power supply
113 magnetic resonance imaging antenna
113' magnetic resonance imaging antenna
114 loop antenna element
114' loop antenna element
115 infrared thermometry sensor
115' infrared thermometry sensor
116 transceiver
118 subject
119 outer surface of subject

120 subject support
122 actuator
124 predetermined direction
125 slices
5 126 computer system
128 hardware interface
130 processor
132 user interface
134 computer storage
10 136 computer memory
140 pulse sequence instructions
142 magnetic resonance data
144 magnetic resonance image
146 thermometry data
15 148 predefined temperature or temperature model
150 control module
152 image reconstruction module
200 acquire the magnetic resonance data by controlling the magnetic resonance imaging system with the pulse sequence instructions
20 202 repeatedly measure at least one surface temperature of the subject with the multiple infrared thermometry sensors
25 204 decision box: is surface temperature above the predefined temperature?
perform a predefined action if the at least one surface temperature is above a predefined temperature
206 decision box: is the acquisition of magnetic resonance data finished?
30 208 end
300 magnetic resonance imaging system
302 support surface
400 enlarged view
402 infrared transparent garment
35 404 path
406 measurement point
600 current leads
602 central region
700 offset region
40

Claims

1. A magnetic resonance imaging antenna (113, 113')
45 comprising a plurality of antenna elements (114, 114'), wherein each of the antenna elements is a loop antenna element, wherein the magnetic resonance imaging antenna further comprises a plurality of infrared thermometry sensors (115, 115'), wherein
50 the magnetic resonance imaging antenna is configured for being positioned adjacent to an external surface of a subject, wherein at least a portion of the multiple infrared thermometry sensors are directed towards the external surface when the magnetic resonance imaging antenna is positioned adjacent to the external surface, for measuring a surface temperature of the subject with the multiple infrared thermometry sensors.
55

2. The magnetic resonance imaging antenna (113, 113') of claim 1, wherein each of the plurality of loop antenna elements have current leads for feeding radio frequency current into or for receiving radio frequency current from the antenna element, wherein at least a subset of the multiple infrared thermometry sensors are positioned such that each sensor of said subset is located adjacent to the current leads of a corresponding antenna element within an offset region which is located offset from a geometrical centre of said corresponding antenna element. 5
3. The magnetic resonance imaging antenna (113, 113') of claim 1, wherein at least a portion of the multiple infrared thermometry sensors are each positioned in a central region (602) of a loop antenna element chosen from the plurality of loop antenna elements. 10
4. The magnetic resonance imaging antenna (113, 113') of claim 1 or 2, wherein the magnetic resonance imaging antenna is configured for functioning as a receive antenna. 20
5. The magnetic resonance imaging antenna (113, 113') of any one of the preceding claims, wherein the magnetic resonance imaging antenna comprises a flexible surface antenna (113), and wherein the flexible surface antenna is configured for being placed in contact with a portion of the outer surface of the subject. 25 30
6. A method of operating a magnetic resonance imaging system (100, 300) for acquiring magnetic resonance data (142) from a subject (118) within an imaging zone (108), wherein the magnetic resonance imaging system comprises a magnetic resonance imaging antenna (113, 113') comprising a plurality of antenna elements (114, 114'), wherein each of the antenna elements is a loop antenna element, wherein the magnetic resonance imaging antenna further comprises multiple infrared thermometry sensors (115, 115'), wherein the magnetic resonance imaging antenna is positioned adjacent to an external surface (119) of the subject, wherein at least a portion of the multiple infrared thermometry sensors are directed towards the external surface when the magnetic resonance imaging antenna is positioned adjacent to the external surface, wherein the method comprises the steps of: 35 40 45 50
 - acquiring (200) the magnetic resonance data by controlling the magnetic resonance imaging system with pulse sequence instructions (140);
 - repeatedly (202) measuring a surface temperature (146) of the subject with the multiple infrared thermometry sensors during acquisition of the magnetic resonance data; and
- performing (204) a predefined action if the surface temperature is above a predefined temperature (148), for reducing the risk of the subject becoming overheated.
7. The method of claim 6, wherein the method further comprises placing an infrared transparent garment (402) on the outer surface of the subject before acquiring the magnetic resonance data.
8. The method of claim 7, wherein the infrared transparent garment is fabricated at least partially from polyethylene foil.
9. A magnetic resonance imaging system (100, 300) for acquiring magnetic resonance data (142) from a subject (118) within an imaging zone (108), wherein the magnetic resonance imaging system comprises:
 - a magnetic resonance imaging antenna (113, 113') as claimed in any one of claims 1-5;
 - a memory (134, 136) containing machine executable instructions (150, 152) and pulse sequence instructions (140), and
 - a processor (130) for controlling the magnetic resonance imaging system, wherein execution of the machine executable instructions causes the processor to:
 - acquire (200) the magnetic resonance data by controlling the magnetic resonance imaging system with the pulse sequence instructions;
 - repeatedly (202) measure at least one surface temperature (146) of the subject with the multiple infrared thermometry sensors during acquisition of the magnetic resonance data; and
 - perform (204) a predefined action if the at least one surface temperature is above a predefined temperature, for reducing the risk of the subject becoming overheated.
10. The magnetic resonance imaging system of claim 9, wherein the magnetic resonance imaging antenna is configured for functioning as a transmit antenna and the infrared thermometry sensors are positioned as defined in claim 2, wherein the magnetic system comprises a RF system (116) for supplying RF power to each of the subset of antenna elements, wherein the predefined action comprises reducing the RF power supplied to a loop antenna element chosen from the subset of antenna elements if an infrared thermometry sensor in the offset region of the loop antenna element measures a surface temperature above the predefined temperature, and wherein the infrared thermometry sensor is chosen from the subset of the multiple infrared thermometry sensors.

11. The magnetic resonance imaging system of any one of claims 9 and 10, wherein the magnetic resonance imaging antenna comprises a subject support (120) configured for supporting the subject on a support surface (302) at least partially within the imaging zone, wherein at least a portion of the antenna elements (114') are arranged within the subject support and adjacent the support surface. 5
12. The magnetic resonance imaging system of any one of claims 9-11, comprising an air cooling system for cooling the subject within the imaging zone with an air flow, wherein the predefined action comprises increasing the air flow if the at least one surface temperature (146) is above the predefined temperature. 10 15
13. The magnetic resonance imaging system of any one of claims 9-12, wherein execution of the machine executable instructions further causes the processor to select the predefined temperature from a table of predefined temperatures using any of the following criteria: subject weight, subject age, subject type, subject size, and combinations thereof. 20
14. The magnetic resonance imaging system of any one of claims 9-13, wherein the predefined action is any one of the following: halt the acquisition of the magnetic resonance data, modify the pulse sequence instructions, increase air ventilation to the subject, and pausing of the acquisition of the magnetic resonance data. 25 30
15. A subject support into which the magnetic resonance imaging antenna of claim 1 is integrated. 35

Patentansprüche

1. Magnetresonanzbildgebungsantenne (113, 113') umfassend eine Vielzahl von Antennenelementen (114, 114'), wobei jedes der Antennenelemente ein Schleifenantennenelement ist, wobei die Magnetresonanzbildgebungsantenne ferner eine Vielzahl von Infrarot-Thermometriesensoren (115, 115') umfasst, wobei die Magnetresonanzbildgebungsantenne konfiguriert ist, um angrenzend an eine Außenfläche einer Person positioniert zu werden, wobei mindestens ein Teil der mehreren Infrarot-Thermometriesensoren auf die Außenfläche gerichtet ist, wenn die Magnetresonanzbildgebungsantenne angrenzend an die Außenfläche positioniert ist, um eine Oberflächentemperatur der Person mit den mehreren Infrarot-Thermometriesensoren zu messen. 40 45 50
2. Magnetresonanzbildgebungsantenne (113, 113') nach Anspruch 1, wobei jedes der Vielzahl von Schleifenantennenelementen Stromleitungen zum Zuführen von Hochfrequenzstrom in das Antennen- 55

element oder zum Empfangen von Hochfrequenzstrom aus dem Antennenelement aufweist, wobei mindestens eine Untergruppe der mehreren Infrarot-Thermometriesensoren derartig positioniert ist, dass sich jeder Sensor der genannten Untergruppe angrenzend an die Stromleitungen eines entsprechenden Antennenelements innerhalb einer Versatzregion befindet, die von einem geometrischen Zentrum des genannten entsprechenden Antennenelements versetzt liegt.

3. Magnetresonanzbildgebungsantenne (113, 113') nach Anspruch 1, wobei mindestens ein Teil der mehreren Infrarot-Thermometriesensoren jeweils in einer zentralen Region (602) eines aus der Vielzahl von Schleifenantennenelementen ausgewählten Schleifenantennenelements positioniert ist.
4. Magnetresonanzbildgebungsantenne (113, 113') nach Anspruch 1 oder 2, wobei die Magnetresonanzbildgebungsantenne konfiguriert ist, um als eine Empfangsantenne zu funktionieren.
5. Magnetresonanzbildgebungsantenne (113, 113') nach einem der vorhergehenden Ansprüche, wobei die Magnetresonanzbildgebungsantenne eine flexible Oberflächenantenne (113) umfasst, und wobei die flexible Oberflächenantenne konfiguriert ist, um in Kontakt mit einem Teil der Außenfläche der Person gebracht zu werden.
6. Verfahren zum Betreiben eines Magnetresonanzbildgebungssystems (100, 300) zum Erfassen von Magnetresonanzdaten (142) aus einer Person (118) innerhalb einer Bildgebungszone (108), wobei das Magnetresonanzbildgebungssystem eine Magnetresonanzbildgebungsantenne (113, 113') umfassend eine Vielzahl von Antennenelementen (114, 114') umfasst, wobei jedes der Antennenelemente ein Schleifenantennenelement ist, wobei die Magnetresonanzbildgebungsantenne ferner eine Vielzahl von Infrarot-Thermometriesensoren (115, 115') umfasst, wobei die Magnetresonanzbildgebungsantenne angrenzend an eine Außenfläche (119) der Person positioniert ist, wobei mindestens ein Teil der mehreren Infrarot-Thermometriesensoren auf die Außenfläche gerichtet ist, wenn die Magnetresonanzbildgebungsantenne angrenzend an die Außenfläche positioniert ist, wobei das Verfahren die folgenden Schritte umfasst:

- Erfassen (200) der Magnetresonanzdaten durch Steuern des Magnetresonanzbildgebungssystems mit Impulssequenzanweisungen (140);
- wiederholtes (202) Messen einer Oberflächentemperatur (146) der Person mit den mehreren Infrarot-Thermometriesensoren während der

- Erfassung der Magnetresonanzdaten; und
 - Durchführen (204) einer vordefinierten Aktion, wenn die Oberflächentemperatur über einer vordefinierten Temperatur (148) liegt, um das Risiko einer Überhitzung der Person zu reduzieren. 5
7. Verfahren nach Anspruch 6, wobei das Verfahren ferner das Platzieren eines infrarot-transparenten Kleidungsstücks (402) auf der Außenfläche der Person vor dem Erfassen der Magnetresonanzdaten umfasst. 10
8. Verfahren nach Anspruch 7, wobei das infrarot-transparente Kleidungsstück zumindest teilweise aus Polyethylenfolie hergestellt ist. 15
9. Magnetresonanzbildgebungssystem (100, 300) zum Erfassen von Magnetresonanzdaten (142) aus einer Person (118) innerhalb einer Bildgebungszone (108), wobei das Magnetresonanzbildgebungssystem Folgendes umfasst:
- eine Magnetresonanzbildgebungsantenne (113, 113') nach einem der Ansprüche 1 bis 5;
 - einen Speicher (134, 136) enthaltend maschinenausführbare Anweisungen (150, 152) und Impulssequenzanweisungen (140), und
 - einen Prozessor (130) zum Steuern des Magnetresonanzbildgebungssystems, wobei das Ausführen der maschinenausführbaren Anweisungen den Prozessor veranlasst zum:
- Erfassen (200) der Magnetresonanzdaten durch Steuern des Magnetresonanzbildgebungssystems mit den Impulssequenzanweisungen; 25
 - wiederholten (202) Messen mindestens einer Oberflächentemperatur (146) der Person mit den mehreren Infrarot-Thermometriesensoren während der Erfassung der Magnetresonanzdaten; und 30
 - Durchführen (204) einer vordefinierten Aktion, wenn die mindestens eine Oberflächentemperatur über einer vordefinierten Temperatur liegt, um das Risiko einer Überhitzung der Person zu reduzieren. 35
10. Magnetresonanzbildgebungssystem nach Anspruch 9, wobei die Magnetresonanzbildgebungsantenne konfiguriert ist, um als eine Sendeantenne zu funktionieren, und die Infrarot-Thermometriesensoren wie in Anspruch 2 definiert positioniert sind, wobei das Magnetsystem ein HF-System (116) zum Zuführen von HF-Energie zu jedem von der Untergruppe von Antennenelementen umfasst, wobei die vordefinierte Aktion das Reduzieren der HF-Leistung, die einem aus der Untergruppe von Antennenelementen ausgewählten Schleifenantennenelement 40
- ment zugeführt wird, umfasst, wenn ein Infrarot-Thermometriesensor in der Versatzregion des Schleifenantennenelements eine Oberflächentemperatur über der vordefinierten Temperatur misst, und wobei der Infrarot-Thermometriesensor aus der Untergruppe der mehreren Infrarot-Thermometriesensoren ausgewählt ist. 45
11. Magnetresonanzbildgebungssystem nach einem der Ansprüche 9 und 10, wobei die Magnetresonanzbildgebungsantenne eine Personenliege (120) umfasst, die konfiguriert ist, um die Person auf einer Auflagefläche (302) zumindest teilweise innerhalb der Bildgebungszone zu lagern, wobei mindestens ein Teil der Antennenelemente (114') innerhalb der Personenliege und angrenzend an die Auflagefläche angeordnet ist. 50
12. Magnetresonanzbildgebungssystem nach einem der Ansprüche 9 bis 11, umfassend ein Luftkühlungssystem zum Kühlen der Person innerhalb der Bildgebungszone mit einer Luftströmung, wobei der vordefinierte Aktion das Erhöhen der Luftströmung umfasst, wenn die mindestens eine Oberflächentemperatur (146) über der vordefinierten Temperatur liegt. 55
13. Magnetresonanzbildgebungssystem nach einem der Ansprüche 9 bis 12, wobei das Ausführen der maschinenausführbaren Anweisungen den Prozessor ferner veranlasst, die vordefinierte Temperatur unter Verwendung von einem der folgenden Kriterien aus einer Tabelle von vordefinierten Temperaturen auszuwählen: Personengewicht, Personenalter, Personentyp, Personengröße und Kombinationen hiervon.
14. Magnetresonanzbildgebungssystem nach einem der Ansprüche 9 bis 13, wobei die vordefinierte Aktion eine der Folgenden ist: Anhalten der Erfassung der Magnetresonanzdaten, Modifizieren der Impulssequenzanweisungen, Erhöhen der Luftventilation für die Person und Unterbrechen der Erfassung der Magnetresonanzdaten.
15. Personenliege, in die die Magnetresonanzbildgebungsantenne nach Anspruch 1 integriert ist.

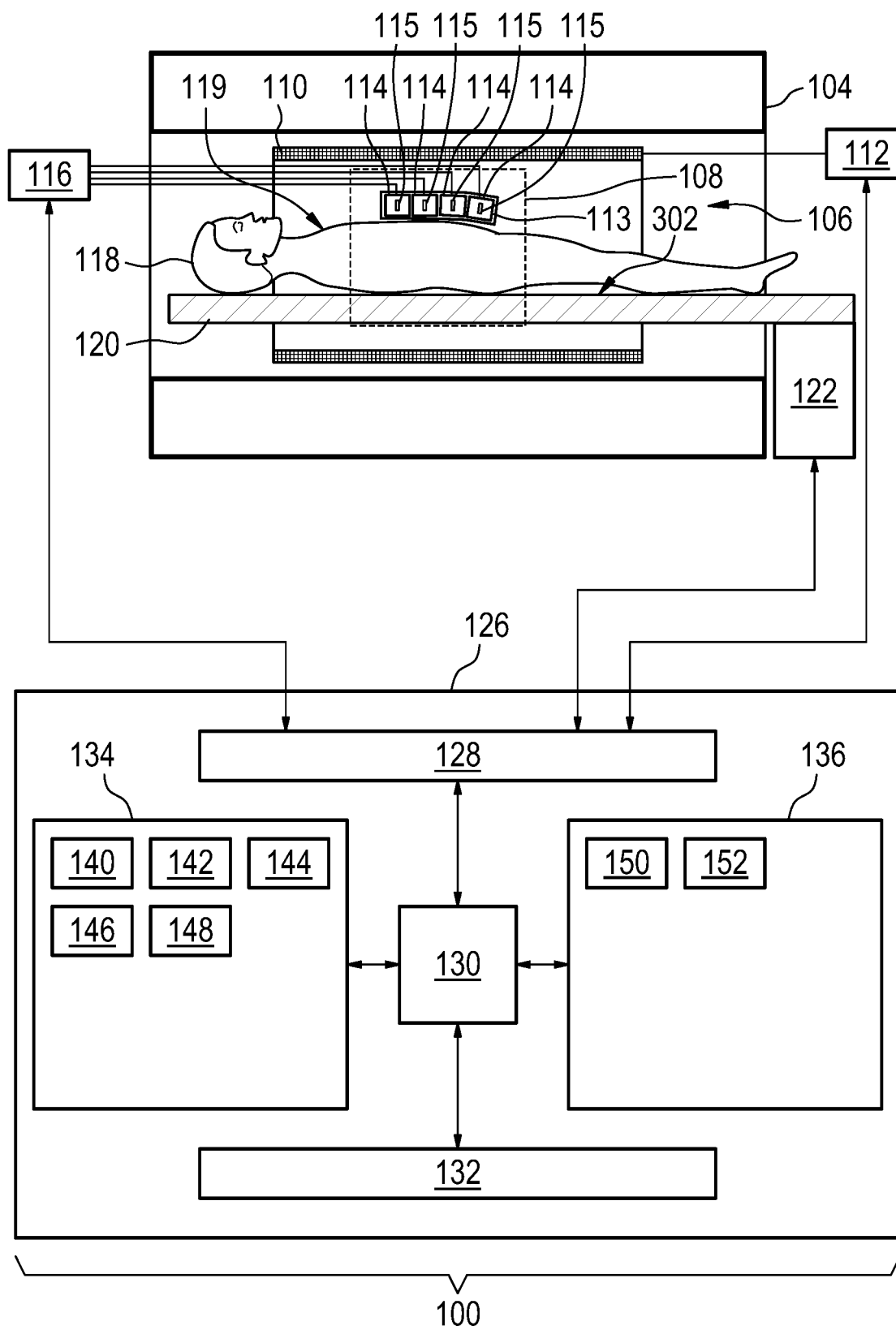
Revendications

1. Antenne d'imagerie par résonance magnétique (113, 113') comprenant une pluralité d'éléments d'antenne (114, 114'), dans laquelle chacun des éléments d'antenne est un élément d'antenne cadre, dans laquelle l'antenne d'imagerie par résonance magnétique comprend en outre une pluralité de capteurs de thermométrie infrarouge (115, 115'), dans

- laquelle l'antenne d'imagerie par résonance magnétique est configurée pour être positionnée au niveau adjacent à une surface externe d'un sujet, dans laquelle au moins une partie des multiples capteurs de thermométrie infrarouge est dirigée vers la surface externe lorsque l'antenne d'imagerie par résonance magnétique est positionnée au niveau adjacent à la surface externe, pour mesurer une température de surface du sujet avec les multiples capteurs de thermométrie infrarouge.
2. Antenne d'imagerie par résonance magnétique (113, 113') selon la revendication 1, dans laquelle chacun de la pluralité des éléments de l'antenne cadre a des conducteurs de courant pour alimenter en courant de radiofréquence ou pour recevoir un courant de radiofréquence de l'élément d'antenne, dans laquelle au moins un sous-groupe des multiples capteurs de thermométrie infrarouge est positionné de sorte que chaque capteur dudit sous-groupe est situé au niveau adjacent aux conducteurs de courant d'un élément d'antenne correspondant dans une région décalée qui est située à un niveau décalé d'un centre géométrique dudit élément d'antenne correspondant.
 3. Antenne d'imagerie par résonance magnétique (113, 113') selon la revendication 1, dans laquelle au moins une partie des multiples capteurs de thermométrie infrarouge sont chacun positionnés dans une région centrale (602) d'un élément d'antenne cadre choisi dans la pluralité d'éléments d'antenne cadre.
 4. Antenne d'imagerie par résonance magnétique (113, 113') selon la revendication 1 ou 2, dans laquelle l'antenne d'imagerie par résonance magnétique est configurée pour fonctionner comme antenne de réception.
 5. Antenne d'imagerie par résonance magnétique (113, 113') selon l'une quelconque des revendications précédentes, dans laquelle l'antenne d'imagerie par résonance magnétique comprend une antenne de surface flexible (113) et dans laquelle l'antenne de surface flexible est configurée pour être placée en contact avec une partie de la surface extérieure du sujet.
 6. Procédé de fonctionnement d'un système d'imagerie par résonance magnétique (100, 300) pour acquérir des données de résonance magnétique (142) d'un sujet (118) dans une zone d'imagerie (108), dans lequel le système d'imagerie par résonance magnétique comprend une antenne d'imagerie par résonance magnétique (113, 113') comprenant une pluralité d'éléments d'antenne (114, 114'), dans lequel chacun des éléments d'antenne est un élément d'antenne cadre, dans lequel l'antenne d'imagerie par résonance magnétique comprend en outre de multiples capteurs de thermométrie infrarouge (115, 115'), dans lequel l'antenne d'imagerie par résonance magnétique est positionnée au niveau adjacent à une surface externe (119) du sujet, dans lequel au moins une partie des multiples capteurs de thermométrie infrarouge est dirigée vers la surface externe lorsque l'antenne d'imagerie par résonance magnétique est positionnée au niveau adjacent à la surface externe, dans lequel le procédé comprend les étapes de :
 - acquisition (200) des données de résonance magnétique en commandant le système d'imagerie par résonance magnétique avec des instructions de séquence d'impulsion (140) ;
 - mesure répétée (202) d'une température de surface (146) du sujet avec les multiples capteurs de thermométrie infrarouge pendant l'acquisition des données de résonance magnétique ; et
 - réalisation (204) d'une action prédéfinie si la température de surface est supérieure à une température prédéfinie (148), pour réduire le risque de surchauffe pour le sujet.
 7. Procédé selon la revendication 6, dans lequel le procédé comprend en outre le placement d'un vêtement transparent aux infrarouges (402) sur la surface extérieure du sujet avant d'acquérir les données de résonance magnétique.
 8. Procédé selon la revendication 7, dans lequel le vêtement transparent aux infrarouges est fabriqué au moins partiellement à partir d'une feuille de polyéthylène.
 9. Système d'imagerie par résonance magnétique (100, 300) pour acquérir des données de résonance magnétique (142) d'un sujet (118) dans une zone d'imagerie (108), dans lequel le système d'imagerie par résonance magnétique comprend :
 - une antenne d'imagerie par résonance magnétique (113, 113') selon l'une quelconque des revendications 1 à 5 ;
 - une mémoire (134, 136) contenant des instructions (150, 152) pouvant être exécutées par une machine et des instructions de séquence d'impulsion (140), et
 - un processeur (130) pour commander le système d'imagerie par résonance magnétique, dans lequel l'exécution des instructions pouvant être exécutées par une machine entraîne, par le processeur :
 - l'acquisition (200) des données de réso-

- nance magnétique en commandant le système d'imagerie par résonance magnétique avec les instructions de séquence d'impulsion ;
- la mesure répétée (202) d'au moins une température de surface (146) du sujet avec les multiples capteurs de thermométrie infrarouge pendant l'acquisition des données de résonance magnétique ; et
 - la réalisation (204) d'une action prédéfinie si l'au moins une température de surface est supérieure à une température prédéfinie, pour réduire le risque de surchauffe pour le sujet.
10. Système d'imagerie par résonance magnétique selon la revendication 9, dans lequel l'antenne d'imagerie par résonance magnétique est configurée pour fonctionner en tant qu'antenne de transmission et les capteurs de thermométrie infrarouge sont positionnés comme le définit la revendication 2, dans lequel le système magnétique comprend un système de RF (116) pour fournir une puissance de RF à chacun des sous-groupes d'éléments d'antenne, dans lequel l'action prédéfinie comprend la réduction de la puissance de RF fournie à un élément d'antenne cadre choisi dans le sous-groupe des éléments d'antenne si un capteur de thermométrie infrarouge dans la région décalée de l'élément d'antenne cadre mesure une température de surface supérieure à la température prédéfinie, et dans lequel le capteur de thermométrie infrarouge est choisi dans le sous-groupe des multiples capteurs de thermométrie infrarouge.
11. Système d'imagerie par résonance magnétique selon l'une quelconque des revendications 9 et 10, dans lequel l'antenne d'imagerie par résonance magnétique comprend un support de sujet (120) configuré pour supporter le sujet sur une surface de support (302) au moins partiellement dans la zone d'imagerie, dans lequel au moins une partie des éléments d'antenne (114') est disposée dans le support de sujet et au niveau adjacent à la surface de support.
12. Système d'imagerie par résonance magnétique selon l'une quelconque des revendications 9 à 11, comprenant un système de refroidissement d'air pour refroidir le sujet dans la zone d'imagerie avec un flux d'air, dans lequel l'action prédéfinie comprend l'augmentation du flux d'air si l'au moins une température de surface (146) est supérieure à la température prédéfinie.
13. Système d'imagerie par résonance magnétique selon l'une quelconque des revendications 9 à 12, dans lequel l'exécution des instructions exécutables par la machine entraînent en outre la sélection par le
- processeur de la température prédéfinie à partir d'un tableau des températures prédéfinies en utilisant l'un quelconque des critères suivants : poids du sujet, âge du sujet, type de sujet, taille du sujet et des combinaisons de ceux-ci.
14. Système d'imagerie par résonance magnétique selon l'une quelconque des revendications 9 à 13, dans lequel l'action prédéfinie est l'une quelconque des suivantes : arrêt de l'acquisition des données de résonance magnétique, modification des instructions de séquence d'impulsion, augmentation de la ventilation à l'air du sujet, et interruption de l'acquisition des données de résonance magnétique.
15. Support de sujet dans lequel l'antenne d'imagerie par résonance magnétique selon la revendication 1 est intégrée.

FIG. 1



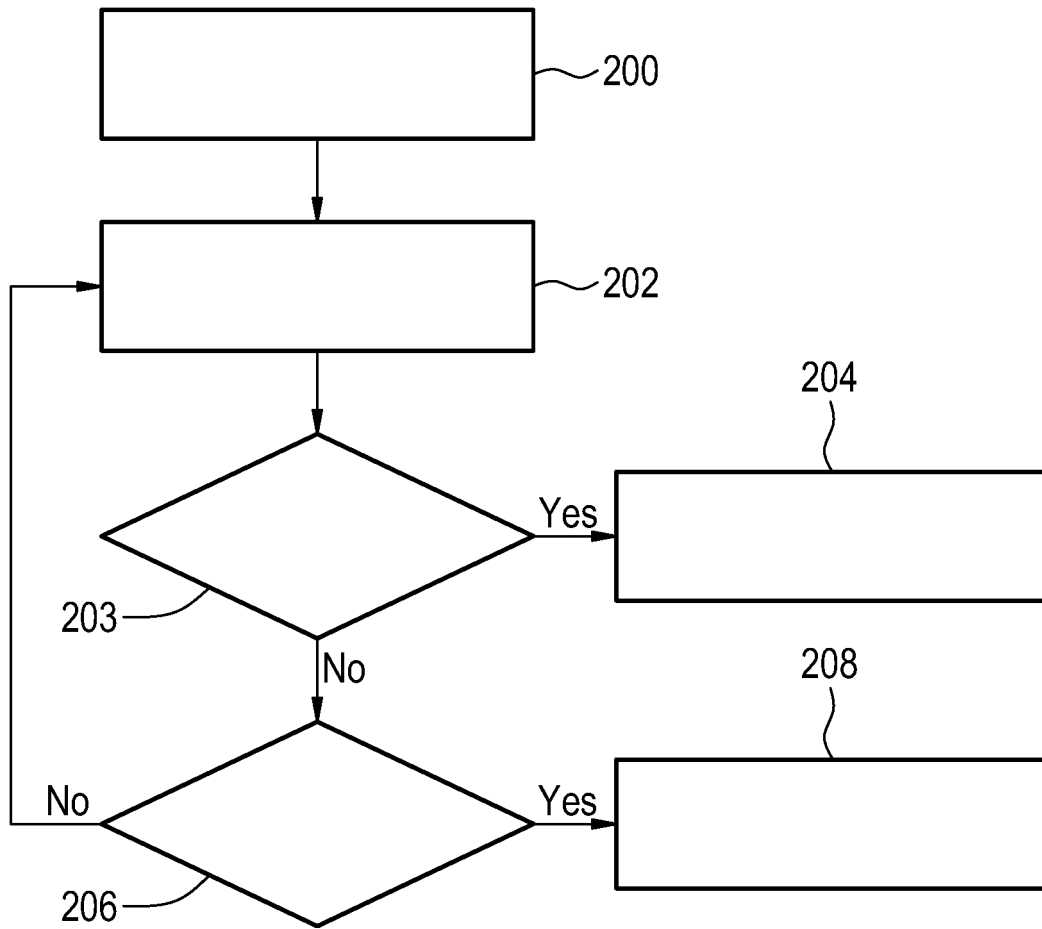


FIG. 3

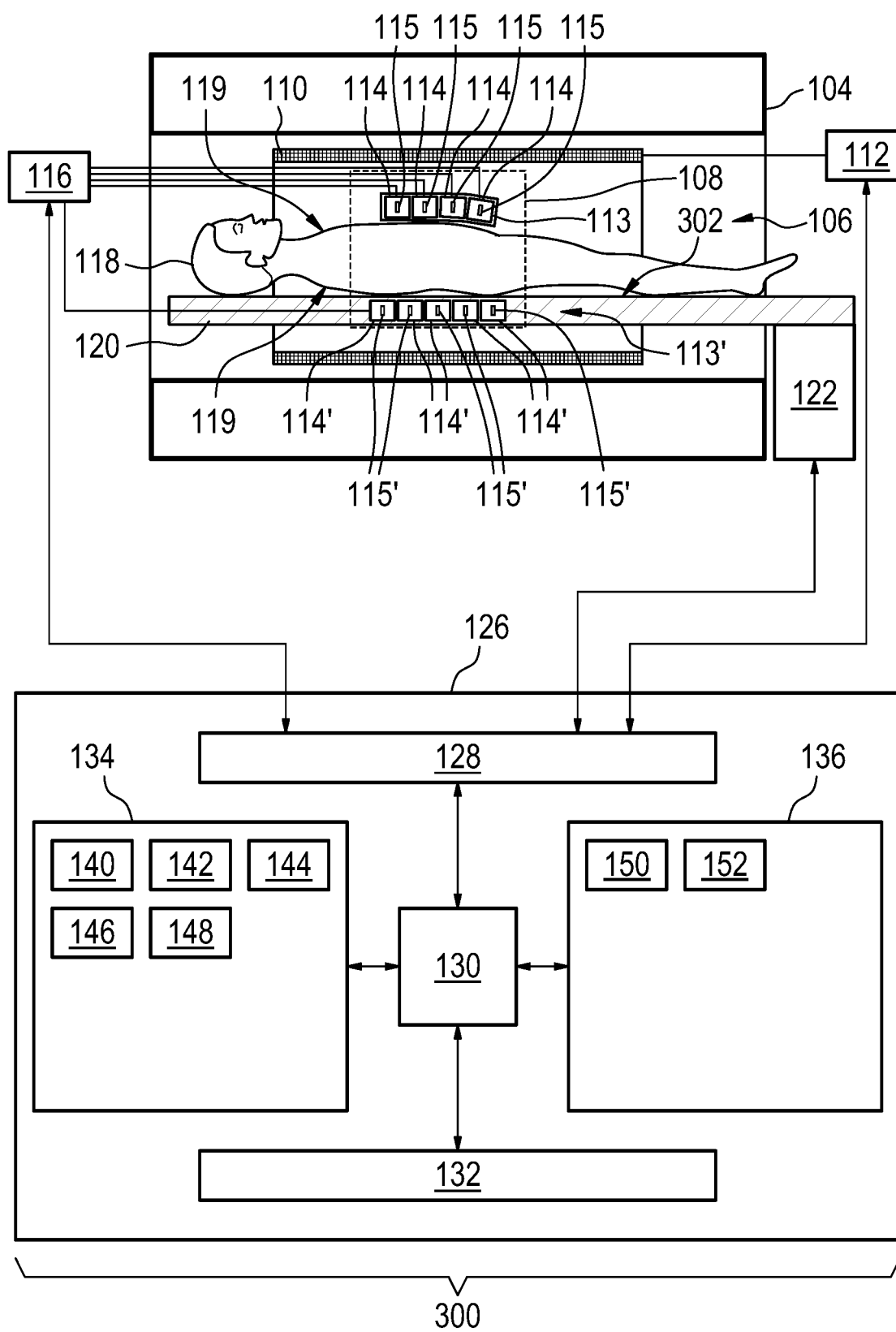


FIG. 4

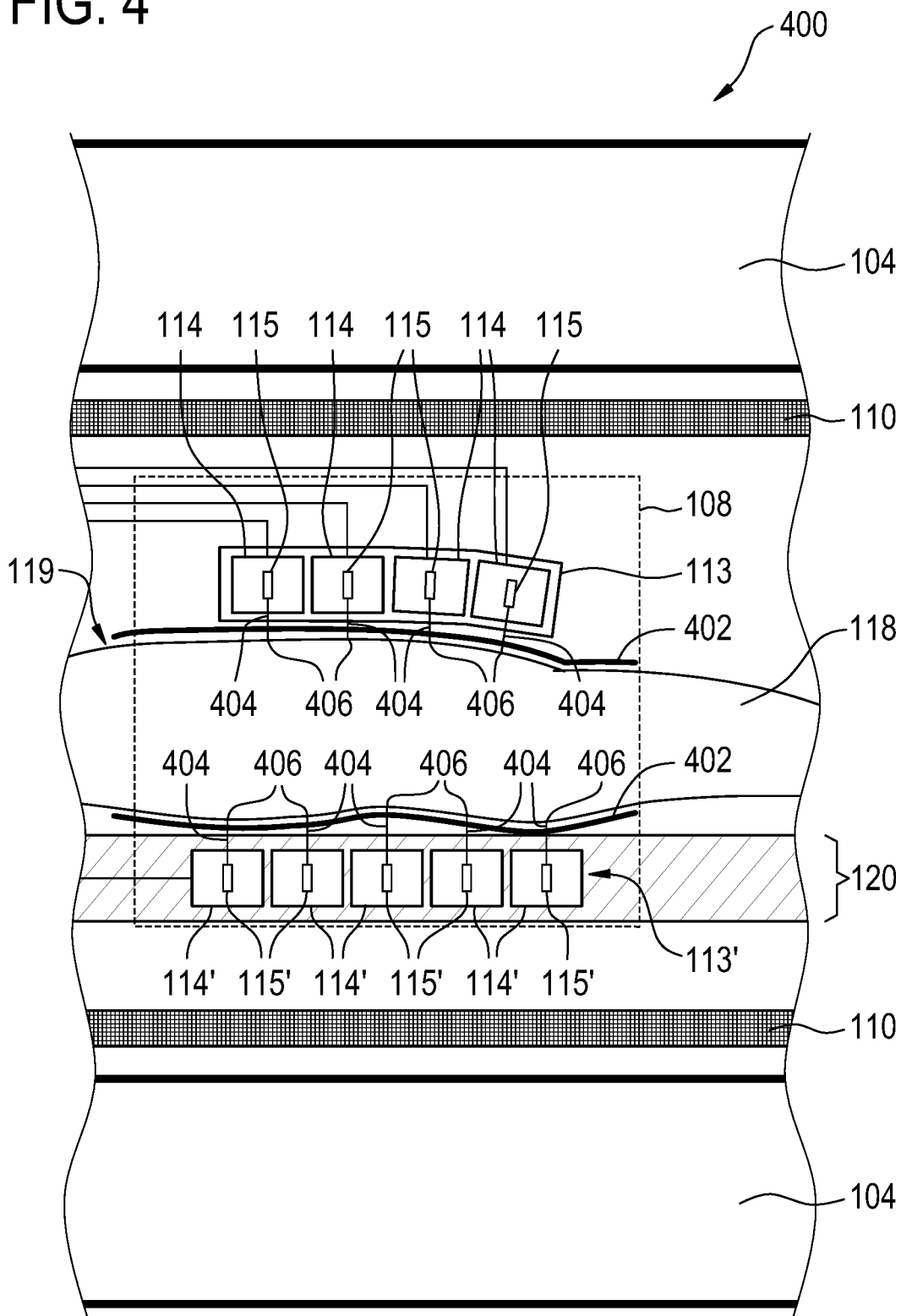


FIG. 5

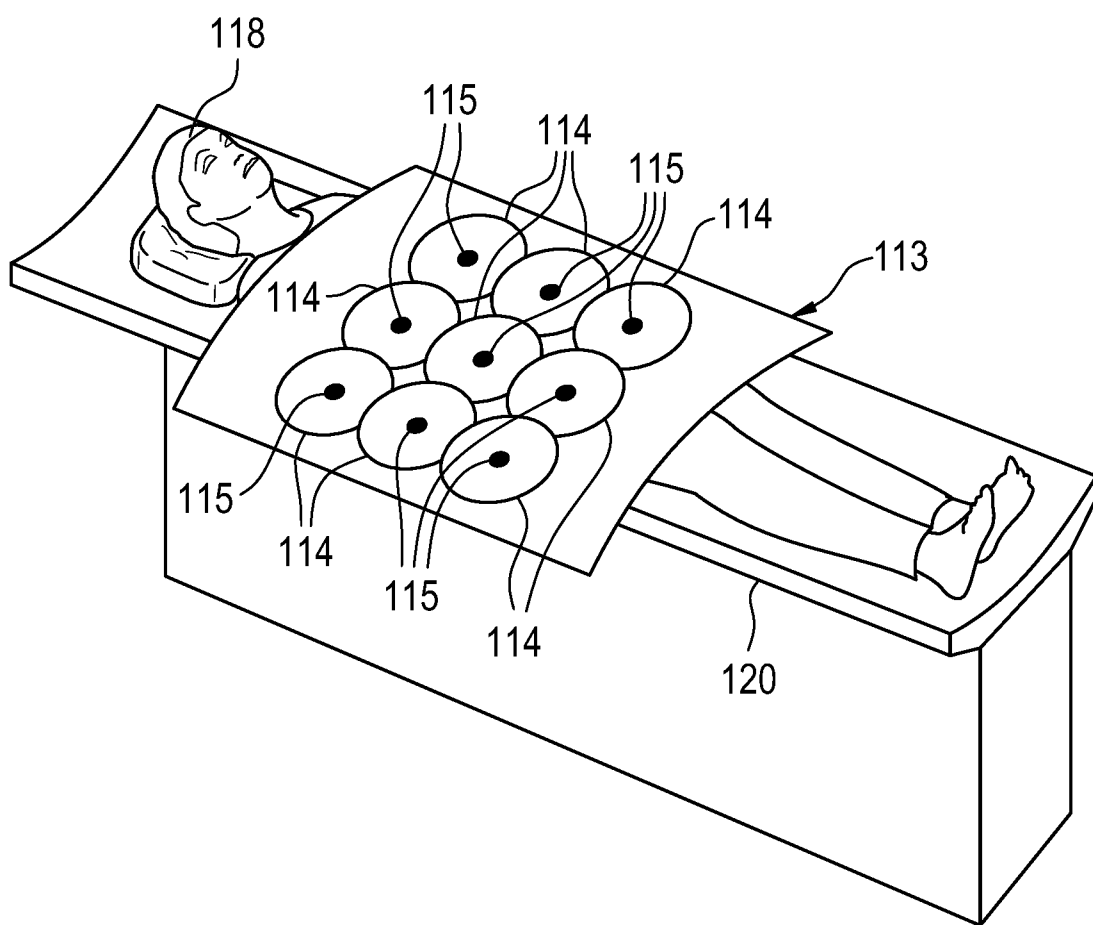


FIG. 6

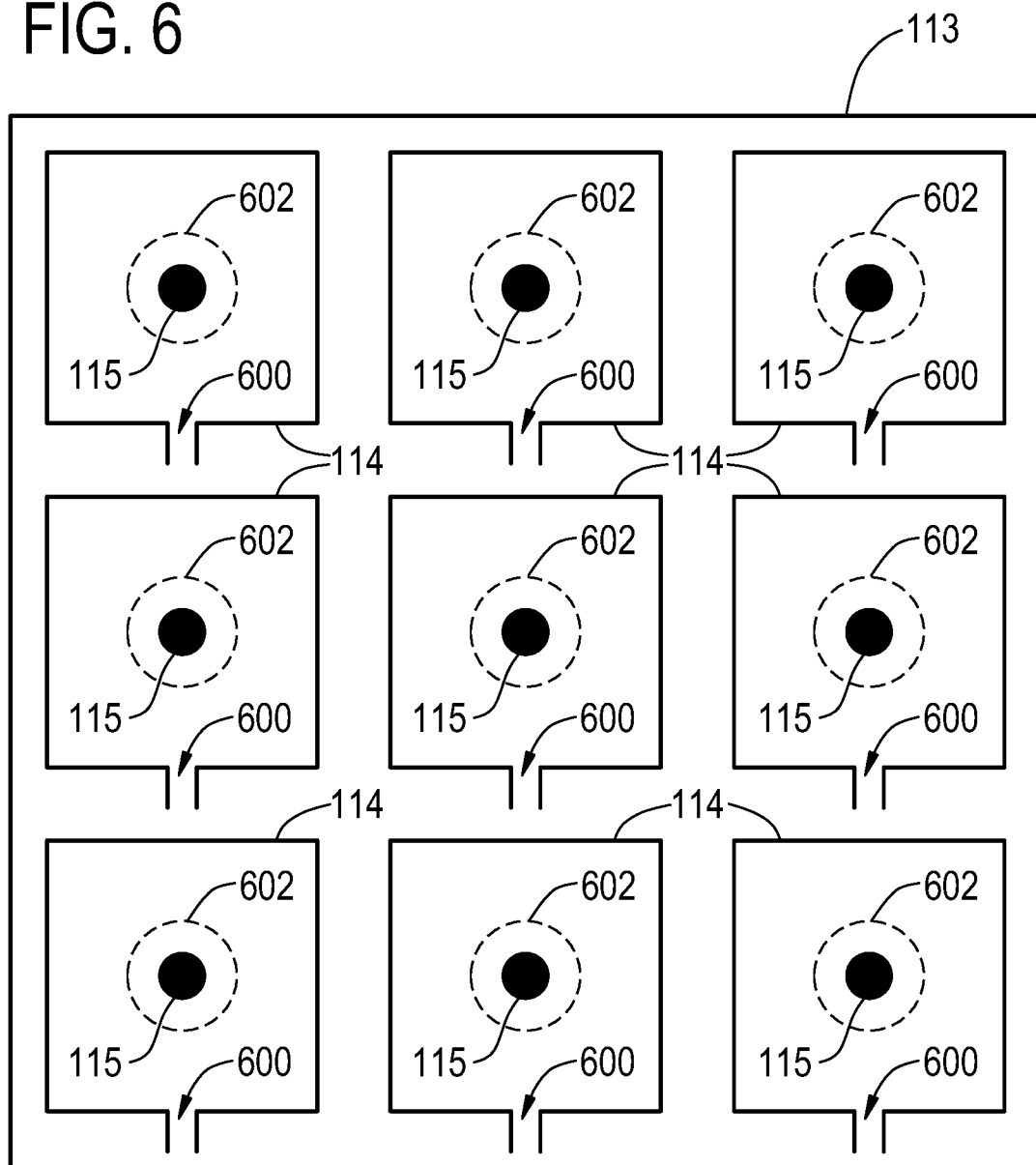


FIG. 7

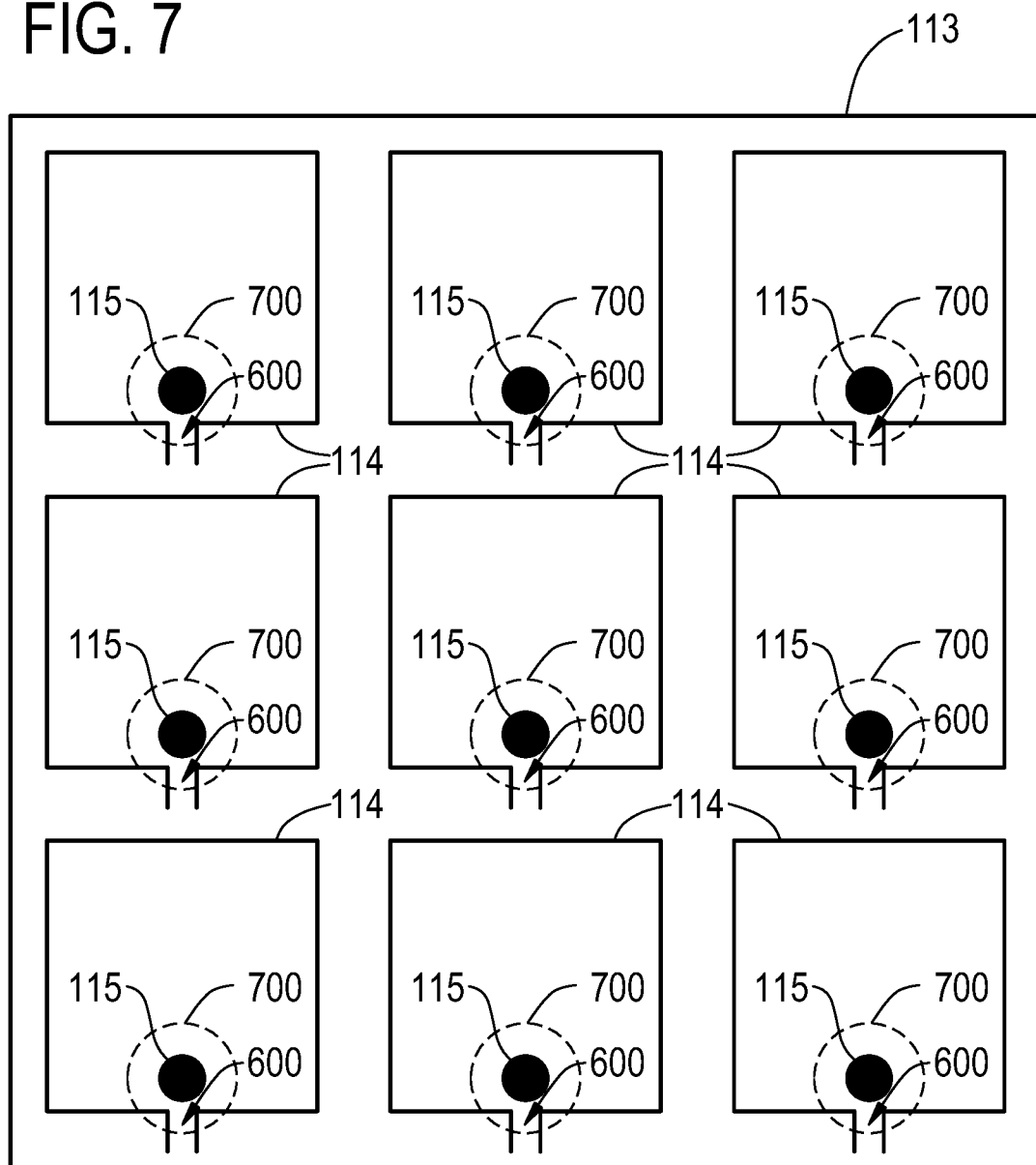
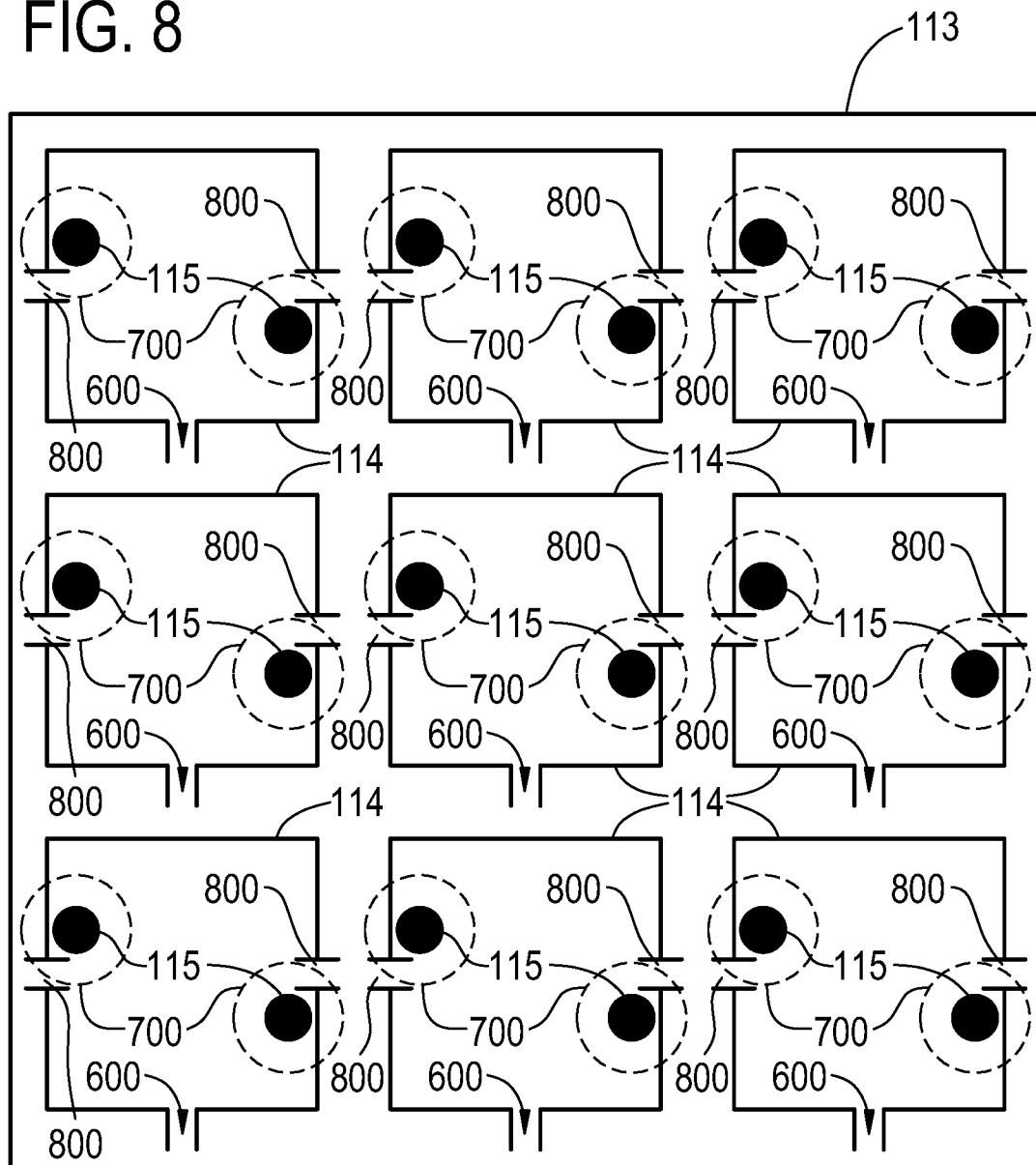


FIG. 8



REFERENCES CITED IN THE DESCRIPTION

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Patent documents cited in the description

- EP 0841576 A [0004]
- JP 2008212437 A [0004]

专利名称(译)	磁共振成像系统，带红外测温传感器		
公开(公告)号	EP3227699B1	公开(公告)日	2018-08-29
申请号	EP2015801856	申请日	2015-11-30
[标]申请(专利权)人(译)	皇家飞利浦电子股份有限公司		
申请(专利权)人(译)	皇家飞利浦N.V.		
当前申请(专利权)人(译)	皇家飞利浦N.V.		
[标]发明人	WEISS STEFFEN		
发明人	WEISS, STEFFEN		
IPC分类号	G01R33/28 G01R33/3415 A61B5/055 A61B5/01 A61B5/00		
CPC分类号	G01R33/288 G01R33/3415 A61B5/0035 A61B5/01 A61B5/055 A61B2560/0266 G01R33/28 G01R33/34015 G01R33/3657 G01R33/3685		
优先权	2014196342 2014-12-04 EP		
其他公开文献	EP3227699A1		
外部链接	Espacenet		

摘要(译)

本发明提供了一种磁共振成像系统 (100,300)，用于从成像区 (108) 内的对象 (118) 采集磁共振数据 (142)。磁共振成像系统包括磁共振成像天线 (113,113#39;)，其包括具有多个红外测温传感器 (115,115#39;) 的多个环形天线元件 (114,114#39;)。磁共振成像天线被配置为邻近对象的外表面 (119) 定位，并且多个红外测温传感器的至少一部分指向外表面。磁共振成像系统还包括存储器 (134,136)，其包含机器可执行指令 (150,152) 和脉冲序列指令 (140)。机器可执行指令使控制系统的处理器：通过用脉冲序列指令控制磁共振成像系统来获取 (200) 磁共振数据;反复 (202) 在获取磁共振数据期间用多个红外测温传感器测量受试者的至少一个表面温度 (146) ;如果所述至少一个表面温度高于预定温度，则执行 (204) 预定动作。

FIG. 1

