

(19) World Intellectual Property Organization
International Bureau



(43) International Publication Date
20 May 2010 (20.05.2010)

PCT

(10) International Publication Number
WO 2010/054863 A1

- (51) International Patent Classification:
A61B 5/00 (2006.01) H04R 1/10 (2006.01)
- (21) International Application Number:
PCT/EP2009/056078
- (22) International Filing Date:
19 May 2009 (19.05.2009)
- (25) Filing Language: English
- (26) Publication Language: English
- (30) Priority Data:
12/272,072 17 November 2008 (17.11.2008) US
- (71) Applicant (for all designated States except US): Sony
Ericsson Mobile Communications AB [SE/SE]; S-221
88 Lund (SE).
- (72) Inventors; and
- (75) Inventors/Applicants (for US only): HAARTSEN, Ja-
cobus [NL/NL]; Bruchterweg 81, NL-7772 BG Harden-
berg (NL). SAMPIMON, Gerrit [NL/NL]; Molenweg 9,
NL-7843 PV Erm (NL).
- (74) Agent: ANDERSSON (LUND), Björn; P.O. Box 793,
S-220 07 Lund (SE).

- (81) Designated States (unless otherwise indicated, for every
kind of national protection available): AE, AG, AL, AM,
AO, AT, AU, AZ, BA, BB, BG, BH, BR, BW, BY, BZ,
CA, CH, CN, CO, CR, CU, CZ, DE, DK, DM, DO, DZ,
EC, EE, EG, ES, FI, GB, GD, GE, GH, GM, GT, HN,
HR, HU, ID, IL, IN, IS, JP, KE, KG, KM, KN, KP, KR,
KZ, LA, LC, LK, LR, LS, LT, LU, LY, MA, MD, ME,
MG, MK, MN, MW, MX, MY, MZ, NA, NG, NI, NO,
NZ, OM, PG, PH, PL, PT, RO, RS, RU, SC, SD, SE, SG,
SK, SL, SM, ST, SV, SY, TJ, TM, TN, TR, TT, TZ, UA,
UG, US, UZ, VC, VN, ZA, ZM, ZW.
- (84) Designated States (unless otherwise indicated, for every
kind of regional protection available): ARIPO (BW, GH,
GM, KE, LS, MW, MZ, NA, SD, SL, SZ, TZ, UG, ZM,
ZW), Eurasian (AM, AZ, BY, KG, KZ, MD, RU, TJ,
TM), European (AT, BE, BG, CH, CY, CZ, DE, DK, EE,
ES, FI, FR, GB, GR, HR, HU, IE, IS, IT, LT, LU, LV,
MC, MK, MT, NL, NO, PL, PT, RO, SE, SI, SK, TR),
OAPI (BF, BJ, CF, CG, CI, CM, GA, GN, GQ, GW, ML,
MR, NE, SN, TD, TG).

Published:

— with international search report (Art. 21(3))

(54) Title: APPARATUS, METHOD, AND COMPUTER PROGRAM FOR DETECTING A PHYSIOLOGICAL MEASURE-
MENT FROM A PHYSIOLOGICAL SOUND SIGNAL

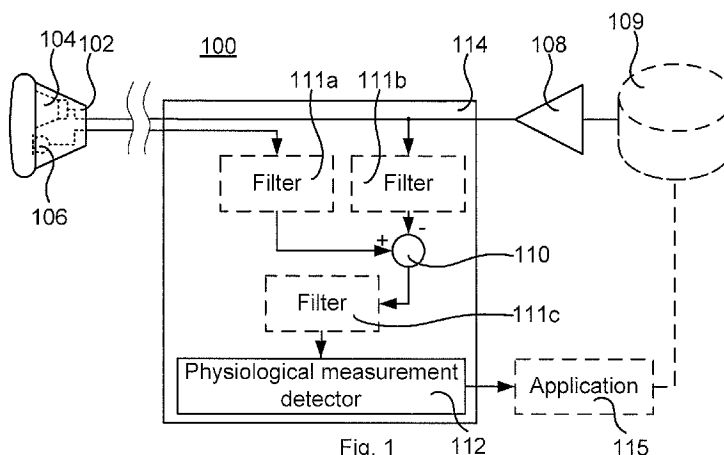


Fig. 1

(57) Abstract: An apparatus is disclosed, comprising a speaker suitable to be applied at a user's ear and enabled to be supplied with an audio signal for rendering; a microphone arranged in vicinity of the speaker to acquire a sound signal from sounds present in the ear of the user; and a signal processor, wherein the signal processor is arranged to subtract the audio signal from the sound signal to provide a physiological sound signal, and the signal processor is further arranged to detect a physiological measurement from the physiological sound signal. A method and a computer program are also disclosed.

WO 2010/054863 A1

TITLE: APPARATUS, METHOD, AND COMPUTER PROGRAM FOR
DETECTING A PHYSIOLOGICAL MEASUREMENT FROM A PHYSIOLOGICAL
SOUND SIGNAL

5

Technical field

The present invention relates to an apparatus, a method, and a computer program for detecting a physiological measurement from a physiological sound signal.

10

Background

Devices for exercising aid and applications in other devices for the same, or applications for other purposes, such as just for amusement have become popular. Such other devices can be portable media players, mobile telephones, and portable digital assistants. Positioning information means, accelerometers, altitude meters, etc. included in such devices may be used for added value. Applications for gaming, exercise aid, log functions, etc. may rely on these measured quantities.

Still, further measured quantities could enhance the devices. It is therefore a desire to add available quantities to measure. However, since the devices are intended to be used by an ordinary user without particular skills and the user normally appreciates gear that is easy to handle, sensors that are used for professional measurements are many times not suitable for these kinds of devices. It is therefore a further desire to provide gear that is easy to use by an ordinary user for the measurements.

20

Summary

The present invention is based on the understanding that an ordinary user is comfortable with using earphones, and that addition of a microphone in an earphone can be used for acquiring sounds from which measurements on physiological sounds present in the user's ear can be made. The physiological sounds are extracted by subtracting sounds provided by the speaker of the earphone. From the physiological sounds, desired quantities and/or qualities are determined, such as heart rate or breathing pattern.

According to a first aspect, there is provided an apparatus comprising a speaker suitable to be applied at a user's ear and enabled to be supplied with an audio signal for rendering; a microphone arranged in vicinity of the speaker to acquire a sound signal from sounds present in the ear of the user; and a signal processor, wherein the signal processor is arranged to subtract the audio signal from the sound signal to provide a

35

physiological sound signal, and the signal processor is further arranged to detect a physiological measurement from the physiological sound signal.

The apparatus may further comprise a filter arranged to filter the sound signal, the audio signal to be subtracted or the physiological sound signal.

5 The apparatus may further comprise an application arranged to control features of the application based on the physiological measurement. The application may be arranged to make music selection based on the physiological measurement, wherein the selected music is comprised in the supplied audio signal. The physiological measurement may comprise a breathing pattern. The signal processor may be arranged
10 to determine a breathing rate from the breathing pattern. The music may be selected based on the music's beat rate such that the music's beat rate is a monotonic function of the breathing rate. The music may be selected based on the music's beat rate such that the music's beat rate is a function of the breathing rate wherein the music's beat rate is increased until a predetermined breathing rate is reached.

15 The physiological measurement may comprise a heartbeat. The signal processor may be arranged to determine a heartbeat rate from the heartbeat. The music may be selected based on the music's beat rate such that the music's beat rate is a monotonic function of the heartbeat rate. The music may be selected based on the music's beat rate such that the music's beat rate is a function of the heartbeat rate
20 wherein the music's beat rate is increased until a predetermined heartbeat rate is reached. The signal processor may be arranged to extract the heartbeat by low pass filtering the physiological sound signal in a low pass filter to provide a heartbeat signal. The low pass filter may have a cutoff frequency between 3 and 10 Hz, preferably between 3 and 5 Hz, preferably 4 Hz.

25 The apparatus may further comprise a second speaker suitable to be provided at the user's other ear, wherein an audio signal provided to the second speaker comprises a sub-signal such that the sound signal comprises a signal component emanating from sound provided at the user's other ear and which sound is modulatedly attenuated by pulsating blood of veins of the user when the sound propagates through the head of the
30 user, and such that the heartbeat is extractable from the signal component. The signal processor may be arranged to extract the heartbeat by low pass filtering the physiological sound signal in a low pass filter to provide the signal component signal. The low pass filter may have a cutoff frequency between 3 and 10 Hz, preferably between 3 and 5 Hz, preferably 4 Hz.

The apparatus may comprise a heart rate estimator arranged to estimate heart rate from the breathing pattern. The physiological measurement may comprise a heartbeat, the signal processor may be arranged to determine a heartbeat rate from the heartbeat, and the apparatus may further be arranged to provide a comparison between the estimated heart rate and the determined heart rate.

The physiological measurement may comprise a heartbeat and a breathing pattern.

According to a second aspect, there is provided a method comprising supplying an audio signal to a speaker suitable to be applied at a user's ear for rendering the audio signal in the user's ear; acquiring a sound signal by a microphone arranged in vicinity of the speaker to acquire the sound signal from sounds present in the ear of the user; subtracting the audio signal from the sound signal to provide a physiological sound signal; and detecting a physiological measurement from the physiological sound signal.

The method may further comprise filtering the sound signal, the audio signal to be subtracted or the physiological sound signal.

The physiological measurement may comprise a breathing pattern, and the method further may comprise controlling features of an application based on the breathing pattern. The controlling of features of the application may comprise selecting music based on the breathing pattern, wherein the selected music is provided to be comprised in the supplied audio signal. The method may further comprise determining a breathing rate from the breathing pattern. The music may be selected based on the music's beat rate such that the music's beat rate is a monotonic function of the breathing rate.

The method may further comprise selecting music based on the breathing pattern, wherein the selected music is provided to be comprised in the supplied audio signal; and determining a breathing rate from the breathing pattern, wherein the selection of music is based on the music's beat rate such that the music's beat rate is increased until a predetermined breathing rate is reached.

The method may further comprise estimating a heart rate from the breathing pattern. The physiological measurement may comprise a heartbeat, the method may further comprise determining a heartbeat rate from the heartbeat; and comparing the estimated heart rate and the determined heart rate, wherein the result of the comparison is used for controlling the features of the application.

The method may further comprise extracting a heartbeat by low pass filtering the physiological sound signal in a low pass filter to provide a heartbeat signal. The low

pass filter may have a cutoff frequency between 3 and 10 Hz, preferably between 3 and 5 Hz, preferably 4 Hz.

The physiological measurement may comprise a heartbeat, and the method may further comprise providing an audio signal which comprises a sub-signal to a second speaker suitable to be applied at the user's other ear, such that the sound signal comprises a signal component emanating from sound provided at the user's other ear and which sound is modulatedly attenuated by pulsating blood of veins of the user when the sound propagates through the head of the user; and detecting the heartbeat from the signal component. The method may further comprise low pass filtering the physiological sound signal in a low pass filter to provide the signal component signal. The low pass filter may have a cutoff frequency between 3 and 10 Hz, preferably between 3 and 5 Hz, preferably 4 Hz.

The physiological measurement may comprise a heartbeat and a breathing pattern.

According to a third aspect, there is provided a computer program comprising program code comprising instructions which when executed by a processor is arranged to cause the processor to perform the method according to the second aspect.

Brief description of drawings

Fig. 1 schematically illustrates an apparatus according to an embodiment.

Fig. 2 is a flow chart illustrating a method according to embodiments.

Fig. 3 is a diagram illustrating functions between provided music beat rate and breathing pattern or heart rate.

Fig. 4 is a block diagram schematically illustrating an application according to an embodiment.

Fig. 5 schematically illustrates a computer readable medium.

Detailed description

Fig. 1 schematically illustrates an apparatus 100 according to an embodiment. The apparatus 100 comprises a speaker arrangement 102, e.g. an earphone, which has a speaker 104 and a microphone 106 arranged together with the speaker 104. The speaker 104 is provided with an audio signal, e.g. music, which preferably is provided by an amplifier 108, which in turn may get the audio content from a media player element 109. As will be demonstrated below, the audio signal can also comprise a sub-signal for heartbeat measurements. The microphone 106, which is arranged to acquire heart or

breathing sounds and of course the audio sound generated by the speaker 104, provides its output signal to a subtractor 110, which subtracts the audio signal from the microphone signal. Optionally, the microphone signal is filtered by a filter 111a. In addition, or alternatively, the audio sound provided by amplifier 108 may be filtered by a filter 111b before input to subtractor 110. The output from the subtractor 110 essentially comprises a heart and/or breathing sound signal since the signal components emanating from the audio sound are deleted. The heart and/or breathing sound signal is provided to a physiological sound detector 112. Here, it should be noted that a filter 111c can be arranged between the subtractor 110 and the physiological sound detector 112 instead of, or in addition to, the filter 111a between the microphone 106 and the subtractor 112 and/or the filter 111b between the amplifier 108 and the subtractor 110. The breathing sound pattern can for example distinguish between breathing through the nose or the mouth. The breathing sound pattern can alternatively or additionally be a measure on breathing rate, e.g. breaths per minute or period between breaths, duty cycle of inhaling and/or exhaling, etc. From the breathing sound pattern, the physical status of a user can be estimated, e.g. during physical exercising. Similar applies for heart sounds, where heart rate and/or amplitude of heart sound can be determined. The subtractor 110, the optional filter(s) 111a, b, c, and the pattern detector 112 can be part of a signal processor 114 performing the functions of the elements 110, 111(a, b, c), 112, for example in analog or digital domain.

In an embodiment, the breathing pattern can be used for controlling an application 115 such that features of the application are adapted to the breathing pattern and/or the heartbeat.

For example, the application can be a music selection application which selects music with a beat rate that depends on for example the breathing rate. This can for example be neat when listening to music while running or jogging, as breathing is related to the physical effort, and also has a relation to step pace. For example, at running exercise, a 4-4 breathing means inhaling during 4 steps and exhaling during 4 steps, and during different parts of an exercise, different breathing strategies can be used, such as changing to 3-3, 2-2, 2-1 etc. If the music is in pace with breathing and thus steps, the exercise can be improved.

Another example is by determining if breathing is nasal or oral. This can be determined on the different sound characteristics the breathing has when the air is flowing in the head. Nasal breathing can then be taken as a sign of low activity

exercising, while oral breathing can be taken as a sign of high activity exercising. Music can then be selected accordingly.

Further another example is by determining if breathing is deep or shallow. This can also be determined from sounds the flowing air is causing in the head, and which
5 sounds can be acquired in the user's ear. An example is to select a lower beat rate on the music if breathing is shallow to calm the user to get into a deep breathing state, which is known to lower heart rate and improve efficiency in exercise. Similarly, if period of breathing is too short to give proper oxygenation in the lungs, lowered music beat rate can improve breathing and exercise.

10 Still another example is a combination of any of the above breathing patterns, where a proper breathing according to a pre-configured or user-configured model is present, but still showing that pace of the exercise can be increased, and therefore an increased beat rate of the music is selected.

Alternatively, or in combination with any of the examples given above, the
15 heart rate and/or intensity of heartbeat sounds can be used for exercising aid, and optionally in combination with the music selection feature.

Of course, the measured breathing pattern and/or heartbeat can also be used in an exercise aid application without controlling any music selection. Similar, the measured breathing pattern and/or heartbeat can also be used in an application without
20 any connection to exercise aid.

The application can of course combine other measured or estimated values and their derivatives too, such as step counter, positioning data, altitude, etc. The settings can be pre-defined or user-defined. The settings can also be down-loadable from a remote location, e.g. over a wireless communication interface such as a cellular
25 telecommunication system. The measured and estimated values can also be saved in a log for post-exercise analysis. Fig. 4 is a block diagram schematically illustrating an example on objects and features of an exercise enhancing application 400. A breathing pattern signal and/or heartbeat signal is input to the application 400, which is controlled by an application engine 402. The application engine 402 is also enabled to receive
30 settings from a settings object 404, which for example can provide settings made by a user, pre-defined settings, or downloaded setting on age, weight, gender, body mass index, exercise limits, exercise type, music function, etc. to the application engine. The application engine can also control one or more function objects 406 for different features. The application 400 can also control other functions or applications, such as a
35 media player, as demonstrated with reference to Fig. 1. The output interface for this

control is preferably controlled by the application engine 402. Here, it should be noted that the example given with reference to Fig. 4 includes a multitude of functions 406. Other examples are any application comprising one or more of the functions given with reference to Fig. 4. The application 400 can for example be implemented as a feature in
5 a mobile phone, a media player, a GPS receiver or a personal digital assistant.

The application can also be independent on physical exercising properties. Breathing can be used for controlling the apparatus 100 on the user's intention, where different breathing patterns are decoded to operation instructions for the apparatus 100, for example changing or pausing music provided by the media player 109.

10 By nature, the heartbeat produces a weak sound in the head of the user with frequency components mainly corresponding to the heart rate. The heartbeat sound signal acquired by the microphone 106 can be amplified, filtered and processed to produce a heart rate value. The filtering can comprise low-pass filtering, since the heartbeat itself normally is within the range of 0.5 to 3 Hz. Since music content
15 normally is very low at these frequencies, a narrow filter can enhance the heart sound signal significantly.

Alternatively, the heartbeat signal is produced by providing a sub-signal to one of the user's ears by a second speaker, which can be done together with e.g. music. Preferably, the sub-signal is at a frequency not discernable by the user, e.g. an ultrasonic
20 or a subsonic frequency should be used. As the sound of the sub-signal propagates through the head of the user to the other ear, the heartbeat will modulate, i.e. provide different attenuation, the sub-signal sound through the pulsation of the blood veins. The sound acquired by the microphone 106 in the other ear will comprise the modulated sub-signal sound. A low-pass filter in case of a subsonic sub-signal, and a high-pass
25 filter in case of an ultrasonic sub-signal can be used to suppress the music signal while detecting the heartbeat. By similar signal processing as demonstrated above, the heart rate can be determined. This approach is particularly suitable for stereo earphones.

Fig. 2 is a flow chart illustrating a method according to embodiments, where hashed lines indicate optional actions. The flow chart is for illustrative purposes, and the
30 order of the actions is not to be interpreted as a sequential order. Instead, the actions are preferably to be considered as real-time objects which can be performed in any order, or in parallel. In an audio supply step 200, an audio signal is provided to a speaker suitable for applying in a user's ear, such as an earphone, for rendering of the audio content of the audio signal. In a sound acquisition step 202, sound present in the user's ear is
35 acquired by a microphone arranged together with the speaker. The sound present in the

user's ear will be a mix of the rendered audio content and sounds generated in the user's head, such as breathing sounds which emanates from air flows in cavities of the head, and heartbeat sounds from blood pulsating in veins in the head according to any of the examples given with reference to Fig. 1. In an optional sound signal filtering step 203, the acquired sound signal can be filtered to enhance the signal, e.g. attenuating frequencies out of frequency range for breathing sounds and/or heartbeat sounds. In an audio signal subtracting step 204, the audio signal is subtracted from the sound signal to extract a breathing signal. In a physiological sound detection step 206, a breathing pattern and/or heartbeat is detected, as demonstrated with reference to Fig. 1.

Optionally, heart rate can be estimated from the detected breathing pattern in a heart rate estimation step 207. Different models for estimating the heart rate from breathing pattern can be used. A user and/or exercise specific model can be used, where one or more characteristics of the breathing pattern are mapped to an expected heart rate. Alternatively, the heart rate can be estimated on the assumption that the faster the breathing rate, the faster the heart rate. Further alternatively, the heart rate can be estimated on the assumption that higher air flow, for example based on the amplitude and/or frequency components of the breathing signal, is mapped to a higher heart rate, and a shallow breathing is mapped to a higher heart rate than deep breathing. The optional heart rate estimation step 207 can be an alternative to the possible heartbeat determination of the physiological sound detection step 206, or a complement for comparison between detected and estimated heart rate, where the comparison can be used as input to an application. In an optional application feature controlling step 209, features of one or more applications can be controlled based on the breathing pattern, alternatively on the estimated heart rate.

Fig. 3 is a diagram illustrating functions between provided music beat rate and breathing pattern or heart rate. For the case of breathing pattern, a determined breathing rate, periodicity, or duty cycle can be used for this type of relation. The solid line illustrates a linear relation between the breathing pattern or estimated heart rate and the music beat rate, while the dot-dashed lines illustrate different non-linear relations. The illustrated lines illustrate monotonic functions for the relation. The application of a monotonic function is particularly suitable when selecting music beat rate from heartbeat rate. Based on breathing pattern, a suitable model out of several non-linear models relating music to heartbeat rate, can be selected. This can further enhance an exercising aid.

The methods according to the present invention are suitable for implementation with aid of processing means, such as computers and/or processors. Therefore, there is provided computer programs, comprising instructions arranged to cause the processing means, processor, or computer to perform the steps of any of the methods according to any of the embodiments described with reference to Fig. 2, in the apparatus. The computer programs preferably comprises program code which is stored on a computer readable medium 500, as illustrated in Fig. 5, which can be loaded and executed by a processing means, processor, or computer 502 to cause it to perform the methods, respectively, according to embodiments of the present invention, preferably as any of the embodiments described with reference to Fig. 2. The computer 502, which can be present in the apparatus as illustrated in Fig. 1, and computer program product 500 can be arranged to execute the program code sequentially where actions of the any of the methods are performed stepwise, or be performed on a real-time basis, where actions are taken upon need and availability of needed input data. The processing means, processor, or computer 502 is preferably what normally is referred to as an embedded system. Thus, the depicted computer readable medium 500 and computer 502 in Fig. 5 should be construed to be for illustrative purposes only to provide understanding of the principle, and not to be construed as any direct illustration of the elements.

20

CLAIMS

1. An apparatus comprising
a speaker suitable to be applied at a user's ear and enabled to be supplied with
5 an audio signal for rendering;
a microphone arranged in vicinity of the speaker to acquire a sound signal from
sounds present in the ear of the user; and
a signal processor, wherein the signal processor is arranged to subtract the
audio signal from the sound signal to provide a physiological sound signal, and the
10 signal processor is further arranged to detect a physiological measurement from the
physiological sound signal.
2. The apparatus according to claim 1, further comprising a filter arranged to
filter the sound signal, the audio signal to be subtracted or the physiological sound
15 signal.
3. The apparatus according to claim 1 or 2, further comprising an application
arranged to control features of the application based on the physiological measurement.
- 20 4. The apparatus according to claim 3, wherein the application is arranged to
make music selection based on the physiological measurement, wherein the selected
music is comprised in the supplied audio signal.
5. The apparatus according to claim 4, wherein the physiological measurement
25 comprises a breathing pattern.
6. The apparatus according to claim 5, wherein the signal processor is arranged
to determine a breathing rate from the breathing pattern
- 30 7. The apparatus according to claim 6, wherein the music is selected based on
the music's beat rate such that the music's beat rate is a monotonic function of the
breathing rate.
8. The apparatus according to claim 6, wherein the music is selected based on
35 the music's beat rate such that the music's beat rate is a function of the breathing rate

wherein the music's beat rate is increased until a predetermined breathing rate is reached.

5 9. The apparatus according to any of claims 5 to 8, comprising a heart rate estimator arranged to estimate heart rate from the breathing pattern.

10 10. The apparatus according to any of claims 1 to 8, wherein the physiological measurement comprises a heartbeat.

11 11. The apparatus according to claim 10, wherein the signal processor is arranged to determine a heartbeat rate from the heartbeat.

12. The apparatus according to claim 11, wherein music of the audio signal is selected based on the music's beat rate such that the music's beat rate is a monotonic
15 function of the heartbeat rate.

13. The apparatus according to claim 11, wherein music of the audio signal is selected based on the music's beat rate such that the music's beat rate is a function of the heartbeat rate wherein the music's beat rate is increased until a predetermined
20 heartbeat rate is reached.

14. The apparatus according to any of claims 10 to 13, wherein the signal processor is arranged to extract the heartbeat by low pass filtering the physiological sound signal in a low pass filter to provide a heartbeat signal.
25

15. The apparatus according to claim 14, wherein the low pass filter has a cutoff frequency between 3 and 10 Hz, preferably between 3 and 5 Hz, preferably 4 Hz.

16. The apparatus according to any of claims 9-14, further comprising a second
30 speaker suitable to be provided at the user's other ear, wherein an audio signal provided to the second speaker comprises a sub-signal such that the sound signal comprises a signal component emanating from sound provided at the user's other ear and which sound is modulatedly attenuated by pulsating blood of veins of the user when the sound propagates through the head of the user, and such that the heartbeat is extractable from
35 the signal component.

17. The apparatus according to claim 9 and any of claims 10 to 16, wherein the apparatus is further arranged to provide a comparison between the estimated heart rate and the determined heart rate.

5

18. A method comprising
supplying an audio signal to a speaker suitable to be applied at a user's ear for rendering the audio signal in the user's ear;
acquiring a sound signal by a microphone arranged in vicinity of the speaker to
10 acquire the sound signal from sounds present in the ear of the user;
subtracting the audio signal from the sound signal to provide a physiological sound signal; and
detecting a physiological measurement from the physiological sound signal.

15

19. The method according to claim 18, further comprising filtering the sound signal, the audio signal to be subtracted or the physiological sound signal.

20

20. The method according to claim 18 or 19, wherein the physiological measurement comprises a breathing pattern, and the method further comprising
controlling features of an application based on the breathing pattern.

25

21. The method according to claim 20, wherein the controlling of features of the application comprises selecting music based on the breathing pattern, wherein the selected music is provided to be comprised in the supplied audio signal.

22. The method according to claim 21, further comprising determining a breathing rate from the breathing pattern.

23. The method according to claim 22, wherein the music is selected based on
30 the music's beat rate such that the music's beat rate is a monotonic function of the breathing rate.

24. The method according to claim 20, further comprising
selecting music based on the breathing pattern, wherein the selected music is
35 provided to be comprised in the supplied audio signal; and

determining a breathing rate from the breathing pattern,
wherein the selection of music is based on the music's beat rate such that the
music's beat rate is increased until a predetermined breathing rate is reached.

5 25. The method according to any of claims 20 to 24, further comprising
estimating a heart rate from the breathing pattern.

10 26. The method according to any of claims 18 to 24, further comprising
extracting a heartbeat by low pass filtering the physiological sound signal in a low pass
filter to provide a heartbeat signal.

 27. The method according to any of claims 18 to 24, wherein the physiological
measurement comprises a heartbeat, and the method further comprises
 providing an audio signal which comprises a sub-signal to a second speaker
15 suitable to be applied at the user's other ear, such that the sound signal comprises a
signal component emanating from sound provided at the user's other ear and which
sound is modulatedly attenuated by pulsating blood of veins of the user when the sound
propagates through the head of the user; and
 detecting the heartbeat from the signal component.

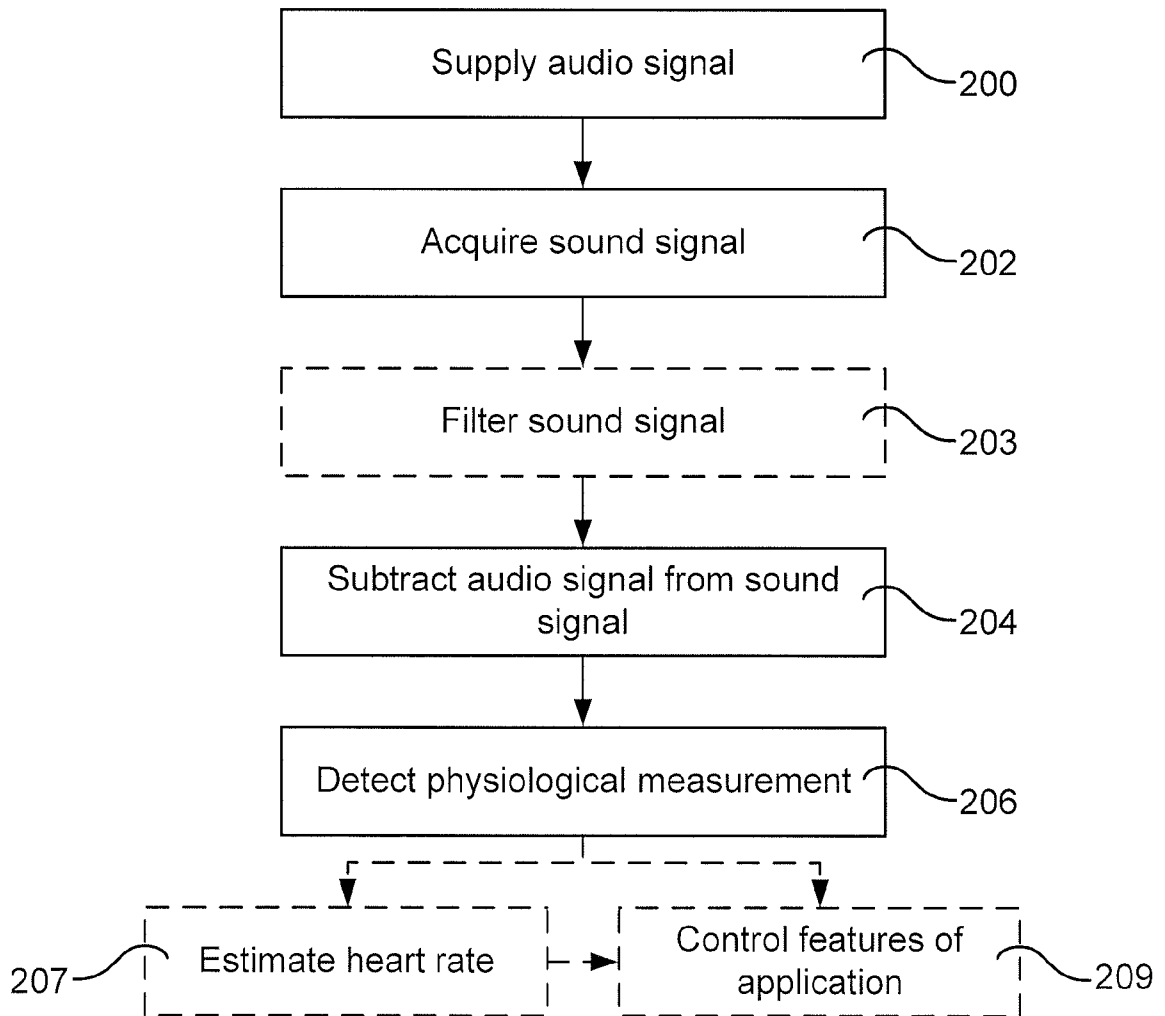
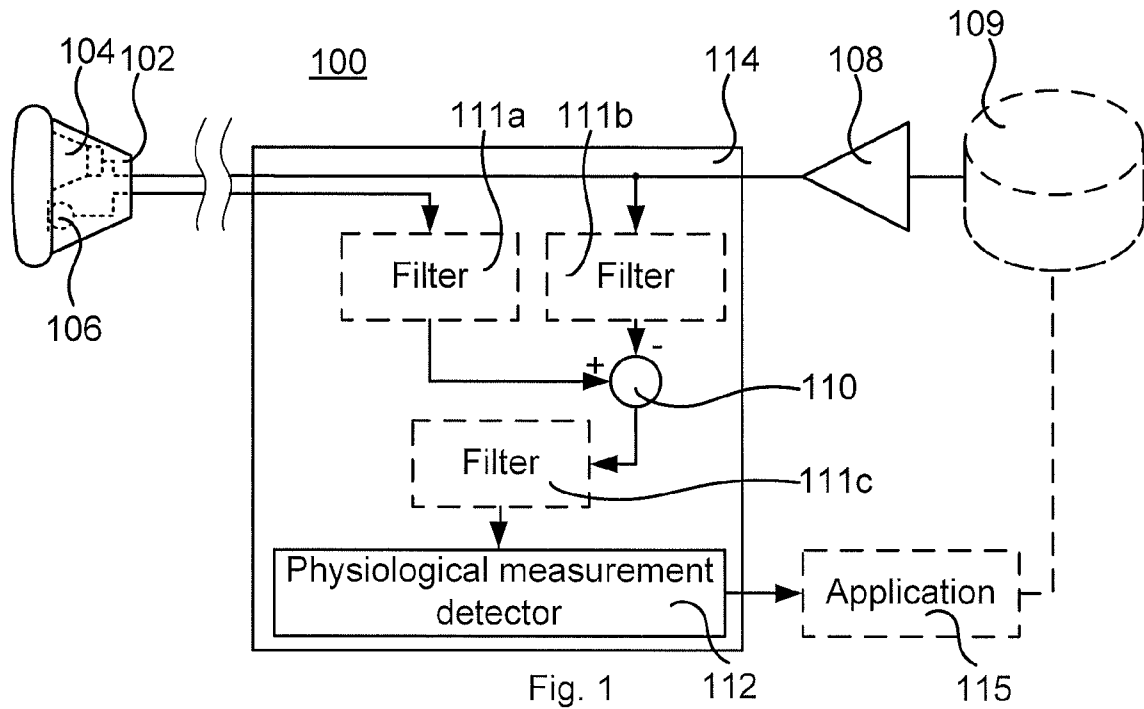
20 28. The method according to claim 27, further comprising low pass filtering the
physiological sound signal in a low pass filter to provide the signal component signal.

25 29. The method according to claim 26 or 28, wherein the low pass filter has a
cutoff frequency between 3 and 10 Hz, preferably between 3 and 5 Hz, preferably 4 Hz.

30 30. The method according to claim 25 and any of claims 26 to 29, the method
further comprising comparing the estimated heart rate and the determined heart rate,
wherein the result of the comparison is used for controlling the features of the
application.

35 31. A computer program comprising program code comprising instructions
which when executed by a processor is arranged to cause the processor to perform the
method according to any of claims 18-30.

1/2



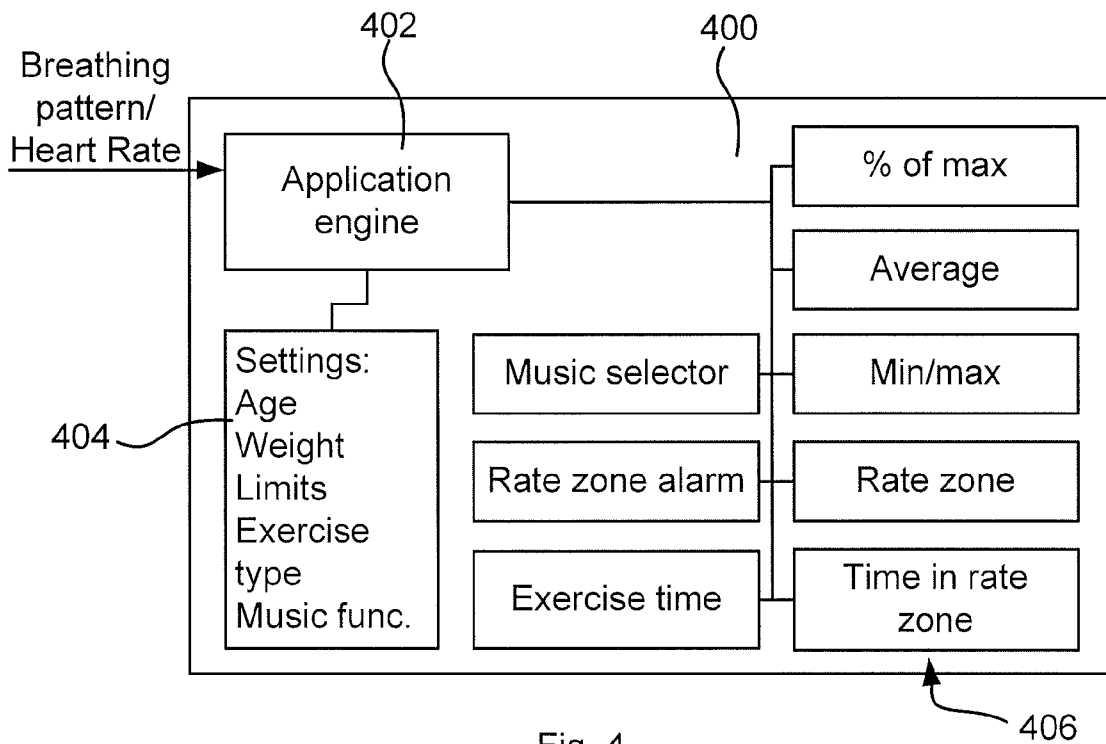
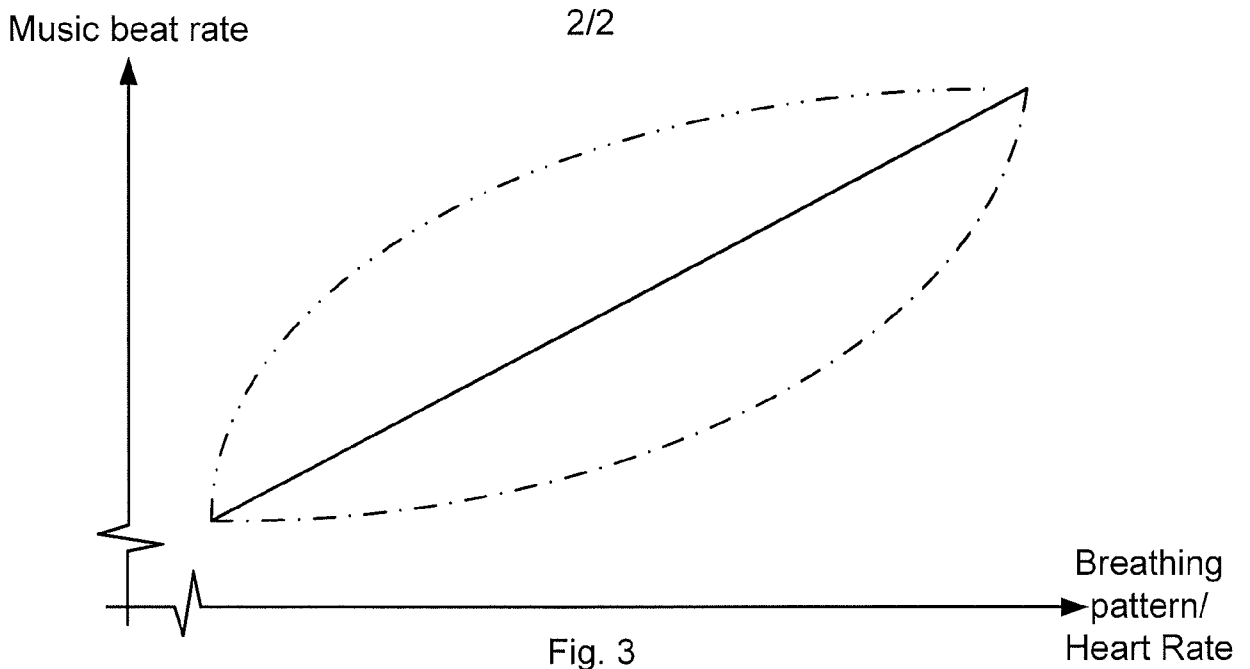


Fig. 4

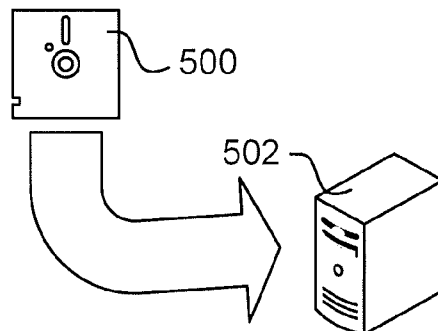


Fig. 5

INTERNATIONAL SEARCH REPORT

International application No
PCT/EP2009/056078

A. CLASSIFICATION OF SUBJECT MATTER

INV. A61B5/00
ADD. H04R1/10

According to International Patent Classification (IPC) or to both national classification and IPC

B. FIELDS SEARCHED

Minimum documentation searched (classification system followed by classification symbols)
A61B A63B H04R

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

Electronic data base consulted during the international search (name of data base and, where practical, search terms used)

EPO-Internal

C. DOCUMENTS CONSIDERED TO BE RELEVANT

Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X	<p>US 2008/146890 A1 (LEBOEUF STEVEN FRANCIS [US] ET AL) 19 June 2008 (2008-06-19)</p> <p>paragraph [0008] - paragraph [0010] paragraph [0014] paragraph [0065] - paragraph [0066] paragraph [0068] - paragraph [0079] paragraph [0105] - paragraph [0109] paragraph [0127] - paragraph [0128] paragraph [0143] paragraph [0149] - paragraph [0150] figures 1-12</p> <p style="text-align: center;">----- -/--</p>	<p>1-6, 10-12, 14-16, 18-22, 25-30</p>

Further documents are listed in the continuation of Box C.

See patent family annex.

* Special categories of cited documents :

- *A* document defining the general state of the art which is not considered to be of particular relevance
- *E* earlier document but published on or after the international filing date
- *L* document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified)
- *O* document referring to an oral disclosure, use, exhibition or other means
- *P* document published prior to the international filing date but later than the priority date claimed

- *T* later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention
- *X* document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone
- *Y* document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art.
- *Z* document member of the same patent family

Date of the actual completion of the international search

29 October 2009

Date of mailing of the international search report

12/11/2009

Name and mailing address of the ISA/

European Patent Office, P.B. 5818 Patentlaan 2
NL - 2280 HV Rijswijk
Tel. (+31-70) 340-2040,
Fax: (+31-70) 340-3016

Authorized officer

Chen, Amy

INTERNATIONAL SEARCH REPORT

International application No

PCT/EP2009/056078

C(Continuation), DOCUMENTS CONSIDERED TO BE RELEVANT		
Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X	<p>US 2006/064037 A1 (SHALON TADMOR [US] ET AL) 23 March 2006 (2006-03-23)</p> <p>paragraph [0075] paragraph [0104] - paragraph [0112] paragraph [0117] - paragraph [0121] paragraph [0232] - paragraph [0249] paragraph [0299] - paragraph [0301] paragraph [0322] - paragraph [0323] paragraph [0329] paragraph [0341] paragraph [0427] - paragraph [0428] figures 1a-4</p>	1-6, 10, 11, 14, 18-22, 25, 26, 31
A	<p>US 2006/107822 A1 (BOWEN ADAM [US]) 25 May 2006 (2006-05-25) paragraph [0045] - paragraph [0079] paragraph [0086] - paragraph [0092]</p>	1-13, 18, 20-26
A	<p>WO 2006/050512 A (PLAIN SIGHT SYSTEMS INC. [US]; COPPI ANDREAS C [US]; COIFMAN RONALD R [US]) 11 May 2006 (2006-05-11)</p> <p>paragraph [0009] - paragraph [0015] paragraph [0020] - paragraph [0029] figures</p>	1-13, 16-18, 20-24, 27-30
A	<p>GB 2 419 946 A (NEC TECHNOLOGIES [GB]) 10 May 2006 (2006-05-10) page 6, line 13 - page 9, line 30 figures 1-3</p>	1, 18
A	<p>US 2002/091049 A1 (HISANO ATSUSHI [US] ET AL) 11 July 2002 (2002-07-11) paragraph [0049] - paragraph [0074] figure 1</p>	1, 18

INTERNATIONAL SEARCH REPORT

Information on patent family members

International application No PCT/EP2009/056078

Patent document cited in search report	Publication date	Patent family member(s)	Publication date
US 2008146890 A1	19-06-2008	EP 2094152 A1 WO 2008088511 A1	02-09-2009 24-07-2008
US 2006064037 A1	23-03-2006	WO 2006033104 A1	30-03-2006
US 2006107822 A1	25-05-2006	US 2009139389 A1	04-06-2009
WO 2006050512 A	11-05-2006	US 2006111621 A1	25-05-2006
GB 2419946 A	10-05-2006	NONE	
US 2002091049 A1	11-07-2002	NONE	

专利名称(译)	用于从生理声音信号中检测生理测量的装置，方法和计算机程序		
公开(公告)号	EP2358264A1	公开(公告)日	2011-08-24
申请号	EP2009779509	申请日	2009-05-19
[标]申请(专利权)人(译)	索尼移动通讯有限公司		
申请(专利权)人(译)	索尼爱立信移动通信AB		
当前申请(专利权)人(译)	索尼爱立信移动通信AB		
[标]发明人	HAARTSEN JACOBUS SAMPIMON GERRIT		
发明人	HAARTSEN, JACOBUS SAMPIMON, GERRIT		
IPC分类号	A61B5/00 H04R1/10 A61B5/0205 A61B5/024 A61B5/08		
CPC分类号	A61B5/6817 A61B5/0205 A61B5/02438 A61B5/0816 A61B5/486 A61B5/6815		
优先权	12/272072 2008-11-17 US		
其他公开文献	EP2358264B1		
外部链接	Espacenet		

摘要(译)

公开了一种装置，包括适于在用户的耳朵处应用并且能够被提供用于呈现的音频信号的扬声器；麦克风设置在扬声器附近，以从用户耳朵中存在的声音中获取声音信号；信号处理器，其中信号处理器用于从声音信号中减去音频信号以提供生理声音信号，并且信号处理器还用于从生理声音信号中检测生理测量值。还公开了一种方法和计算机程序。