



(12) **EUROPEAN PATENT APPLICATION**

(43) Date of publication:
07.11.2018 Bulletin 2018/45

(51) Int Cl.:
A61B 5/00 (2006.01) **A61B 5/0476** (2006.01)
A61B 5/048 (2006.01) **G16H 50/20** (2018.01)

(21) Application number: **17175004.5**

(22) Date of filing: **08.06.2017**

(84) Designated Contracting States:
AL AT BE BG CH CY CZ DE DK EE ES FI FR GB GR HR HU IE IS IT LI LT LU LV MC MK MT NL NO PL PT RO RS SE SI SK SM TR
Designated Extension States:
BA ME
Designated Validation States:
MA MD

(72) Inventors:
• **CHANG, Chia-Chi**
116 Taipei City (TW)
• **LIN, Pei-Chen**
300 Hsinchu City (TW)

(74) Representative: **Lang, Christian**
LangPatent Anwaltskanzlei
IP Law Firm
Rosenheimer Straße 139
81671 München (DE)

(30) Priority: **04.05.2017 TW 106114720**

(71) Applicant: **A-Neuron Electronic Corp.**
Zhubei City, Hsinchu 30273 (TW)

(54) **BRAIN ACTIVITY ANALYSIS METHOD AND APPARATUS THEREOF**

(57) There is a brain activity analysis method and apparatus disclosed, which is based on a nonlinear waveform decomposition technology, wherein the changes of the intrinsic features in brain waves are decomposed and demodulated to extract the modulation signals of the components, including the frequency-modulation signals and the amplitude-modulation signals. It further uses a feature mask to determine whether to pro-

ceed further decomposition and demodulation of the extracted modulation signals. If not, the multidimensional changes of the intrinsic features are obtained according to the feature mask. Then, quantitation and identification is performed to obtain the status of brain function. It not only effectively increases the accuracy of the identification but also uses the feature mask to obviously reduce the complexity and the load of computation.

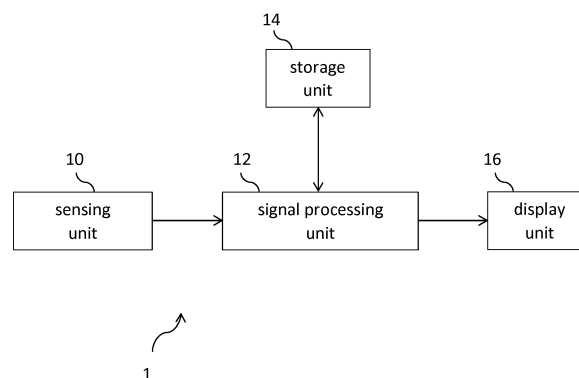


FIG.1

Description

[0001] This application claims priority for Taiwan patent application no. 106114720 filed on May 4, 2017, the content of which is incorporated by reference in its entirety.

BACKGROUND OF THE INVENTION

Field of the Invention

[0002] The present invention relates to a brain wave analysis technology, particularly to a brain activity analysis method able to evaluate brain activity and an apparatus thereof.

Description of the Related Art

[0003] The conventional brain wave analysis includes waveform analysis, time-frequency analysis, complexity analysis, etc. The result of time-frequency analysis is an important reference in the related field. However, the evaluation of brain activity based on time-frequency analysis is constrained by the limitations of spectral calculation, such as the mathematic assumption, timescale resolution, information distortion, and harmonics influences. Thus, the applicability of time-frequency analysis is greatly degraded. Further, the current time-frequency analysis technology is less likely to analyze the result of multiplication but can only analyze the result of linear addition.

[0004] The conventional seizure detection, which based on time-frequency analysis method, adopts frequency measurement (by increasing a 30-40Hz oscillation component) and amplitude measurement for seizure detection. In general, the changes of a physiological signal, such as brain electrical signal, contain various physiological mechanisms and relevant interferences. The mathematic neural network model consists of addition and multiplication within multiple layer structure. The brain wave signal is resulting from the neural network and is sensed by the electroencephalography. The conventional technology of brain wave analysis is to analyze the "features appearing in neuron operation" or the "brain function states corresponding to brain waves". However, the existing technology is hard to analyze the signal modulation of multiplication and is limited for relevant applications.

[0005] The prior art of published related patents respectively have different disadvantages. The U.S. patent No. 6,480,743 disclosed a "system and method for adaptive brain stimulation", which is intended to be used as a treatment of neurological diseases. The patent adopts a half-wave analysis technology to acquire the parameters for setting the waveform of the electric stimulus of treatment. The parameter setting of the prior art is mainly according to the fundamental characteristics of primitive brain wave signal. Thus, the result of identification is mainly affected by the interferences of the primitive brain

wave signal. The U.S. patent No. 8,131,352 disclosed a "system and method for automatically adjusting detection thresholds in a feedback-controlled neurological event detector", which adopts the amplitude features of the primitive brain wave with a threshold value for the event detection. However, the amplitude features consists of various physiological information and is much sensitive to the bias of the target signal, which might cause the detection error. The U.S. patent No. 6,810,285 disclosed "seizure sensing and detection using an implantable device", which adopts waveform morphology analysis (including time-domain analysis and feature extraction analysis) to detect neurological events. All the operations thereof are based on the primitive waveform of the brain wave signal. Thus, the detection results are sensitive to the interferences of waveform distortion caused by noises. Further, the accuracy thereof is limited by the fact that a part of regulations of neurological functions are presented in the modulated signals and unlikely to be evaluated and estimated with the features of the primitive waveform. A Taiwan patent No. I487503 disclosed "an automatic sleep staging device, which uses entropy analysis to evaluate the brain activity". However, the prior art cannot deal with the changes of the time-frequency features of brain wave signal but can only estimate the complexity feature. Besides, the prior art adopts the filtering and smoothing respectively before and after the main waveform processing, which might reduce the key intrinsic characteristics and practically cause detection error.

[0006] In order to evaluate brain functionality and breakthrough limitations of the conventional technology, the present invention constructs a novel algorithm to implement a brain activity analysis method and an apparatus thereof to analyze the features appearing in neuron operation and the brain function status, named brain activity, corresponding to the brain waves.

SUMMARY OF THE INVENTION

[0007] The primary objective of the present invention is to provide a brain activity analysis method and an apparatus thereof, which decomposes and analyzes frequency modulations and amplitude modulations to construct a multilayer and multidimensional feature space presenting the nonstationary features in brain activities.

[0008] Another objective of the present invention is to provide a brain activity analysis method and an apparatus thereof, which uses a feature mask to greatly reduce the computation complexity of the conventional decomposition technology and thus obviously reduce computation loading, whereby to improve the feasibility of the brain wave analysis technology.

[0009] A further objective of the present invention is to provide a brain activity analysis method and an apparatus thereof, which can improve the detection rate of the brain wave analysis.

[0010] In order to achieve the abovementioned objectives, the present invention proposes a brain activity anal-

ysis method, which comprises several steps: sensing at least one brain electrical signal; using a nonstationary decomposition method to acquire a plurality of sub-signals corresponding to intrinsic feature components; demodulating each of the sub-signals to generate modulation signals respectively corresponding to the sub-signals; undertaking recursive iterations, wherein a feature mask is used to determine whether to proceed further decomposition and demodulation of the acquired modulation signals; if yes, perform decomposition and demodulation until the iteration number, which is determined by the feature mask, has been reached; if no, i.e. the decomposition and demodulation is completed, the process directly proceeds to the next step: using the feature mask to select modulation signals of interest from all the modulation signals as feature modulation signals, and undertaking quantitation processes and identification processes of the feature modulation signals to obtain an analysis result corresponding to the brain electrical signal.

[0011] In the method of the present invention, the modulation signals include frequency-modulation parts and amplitude-modulation parts.

[0012] The present invention also proposes a brain activity analysis apparatus, which comprises at least one sensing unit, a signal processing unit, and a display unit. The sensing unit collects the brain wave signal of a subject to acquire at least one brain electrical signal. The signal processing unit is in communication with the sensing unit to receive the brain electrical signal and uses the abovementioned method to decompose and demodulate the brain electrical signal. According to a feature mask, the signal processing unit determines whether to proceed the recursive iteration of the processing or select modulation signals of interest from all the modulation signals as feature modulation signals. After acquiring the feature modulation signals, the signal processing unit performs quantitation processes and identification processes of all the feature modulation signals to obtain an analysis result corresponding to the brain electrical signal. Then, the signal processing unit presents the analysis result as brain activity on a display unit.

[0013] In one embodiment, the brain activity analysis apparatus further comprises a storage unit electrically connected with the signal processing unit to store the signals, data, and results, which are processed or generated by the signal processing unit.

[0014] Below, embodiments are described in detail in conjunction with the accompanying drawings to make easily understood the objectives, technical contents and accomplishments of the present invention.

BRIEF DESCRIPTION OF THE DRAWINGS

[0015]

Fig.1 is a block diagram schematically showing a brain activity analysis apparatus according to one embodiment of the

Fig.2

5 Fig.3(a)

Fig.3(b)

10

Fig.3(c)

15

20 Fig.3(d)

25 Fig.3(e)

Fig.3(f) is

30

Figs.4(a)-4(e)

35

40

45

50

55

present invention;

is a flowchart of a brain activity analysis method according to one embodiment of the present invention;

is a diagram showing a primitive brain wave signal;

is a diagram schematically showing that a brain electrical signal is decomposed into a plurality of sub-signals carrying intrinsic feature components according to one embodiment of the present invention;

is a diagram schematically showing that the sub-signals are demodulated into modulation signals each containing a frequency-modulation part and an amplitude-modulation part according to one embodiment of the present invention;

is a diagram schematically showing the signals generated after decomposition and demodulation has been proceeded three times according to one embodiment of the present invention;

is a diagram schematically showing the signals determined by a feature mask according to one embodiment of the present invention;

a diagram schematically showing that the modulation signals of interest are selected from all the modulation signals according to one embodiment of the present invention; and

are diagrams schematically showing the signals generated in sequential cycles of decomposing and demodulating the brain electrical signal measured during normal condition and seizure according to one embodiment of the present invention, wherein the feature mask is $M = x(FM[2], AM[1(FM[1,2], AM[1,2]), 2])$.

DETAILED DESCRIPTION OF THE INVENTION

[0016] The brain activity analysis method and apparatus of the present invention is corresponding to the fundamental operation architecture of a neural network, using a nonlinear waveform decomposition technology to explore features of variations of different modulations and work out multilayer-multidimensional intrinsic variations, whereby to provide a multidimensional and low-distortion analysis technology of neurological function, wherefore the accuracy of using brain waves to diagnose neurological diseases is increased.

[0017] Refer to Fig.1 a block diagram schematically showing a brain activity analysis apparatus according to one embodiment of the present invention. The brain ac-

tivity analysis apparatus 1 of the present invention comprises a sensing unit 10 detecting the brain wave signal of a subject to acquire a brain electrical signal; a signal processing unit 12 in communication with the sensing unit 10; a storage unit 14 electrically connected with the signal processing unit 12; and a display unit 16 electrically connected with the signal processing unit 12. The signal processing unit 12 is an application-specific integrated circuit (ASIC), a microcontroller unit (MCU) or a micro-processor. The signal processing unit 12 receives the brain electrical signal and performs calculations of the intrinsic feature components to obtain an analysis result corresponding to the brain electrical signal, such as the status of brain activity. The models, data, and signals used in processing and analysis and the results are stored in the storage unit 14, which may be an external or built-in storage device. The display unit 16 presents the information output by the signal processing unit 12 and the results of evaluating the status of brain activity.

[0018] After the fundamental architecture of the apparatus of the present invention has been described above, the brain activity analysis method of the present invention will be fully described below. Refer to Fig. 2 a flowchart of a brain activity analysis method according to one embodiment of the present invention, and refer to Fig. 1 again. The brain activity analysis method of the present invention comprises Steps S10-S24. In Step S10, use the sensing unit 10 to measure the brain wave of at least one subject to acquire at least one brain electrical signal, as shown in Fig. 3(a). The brain electrical signal may be an electroencephalography (EEG) signal, an intracranial electroencephalogram (iEEG) signal, or an electrocorticography (ECoG) signal. The brain electrical signal is transmitted to the signal processing unit 12 and processed and analyzed in Steps S12-S24.

[0019] In Step S12, use a nonstationary decomposition method, such as the empirical mode decomposition (EMD) method, to decompose the brain electrical signal to acquire a plurality of sub-signals carrying intrinsic feature components, as Components 1-7 shown in Fig. 3(b). In Step S14, demodulate each of the sub-signals, wherein a normalization operation is used to decompose the sub-signals, which respectively carry different intrinsic feature components, to acquire modulation signals respectively corresponding to the sub-signals. The modulation signals include frequency-modulation parts and amplitude-modulation parts. The Layer 1 signal shown in Fig. 3(c) includes the frequency-modulation parts ($W_k(t)$, $k=1-7$) and the amplitude-modulation parts ($A_i(t)$, $i=1-7$), which are obtained via decomposing every sub-signal. In Step S16, perform recursive iteration, wherein a preset feature mask is used to determine whether to perform recursive iteration of the acquired modulation signal (including the frequency-modulation parts and the amplitude-modulation parts), i.e. determine whether to perform a further decomposition-demodulation process of the acquired signals. If no, the process directly proceeds to Step S20. If yes, the process proceeds to Step

S18: continue decomposition and demodulation of the signals. The details of the decomposition and demodulation in Step S18 are respectively identical to Step S12 and Step S14. After Step S18 is completed, the process returns to Step S16 for determining whether to proceed a further decomposition-demodulation process of the signals until the number of decomposition and demodulation has reached the number determined by the feature mask. The number of recursive iteration (the number of decomposition and demodulation of signals) is exactly the number of the layers that the signal is decomposed into. The number of recursive iteration required to analyze the feature is dependent on the characteristics of the signal. In this embodiment, the components of Layer 1 are further decomposed and demodulated for the second time and the third time to generate the Layer 2 modulation signals shown in Fig. 3(c) and the Layer 3 modulation signals shown in Fig. 3(d).

[0020] The number of recursive iteration and the signal features determine feature components. Therefore, in Step S20, set a feature mask M to determine the feature components. As shown in Fig. 3(e) and Fig. 3(f), the feature mask M is used to select modulation signals of interest as feature modulation signals from Layer 1 modulation signals, Layer 2 modulation signals and Layer 3 modulation signals. The feature modulation signals are to be used in the succeeding calculation to obtain the multidimensional variation of the intrinsic features of the brain wave. In Step S22, perform quantitation processes of the features of interest, such as calculation of power densities, instantaneous frequencies, or averaged periods of the features of interest. In Step S24, use a classification model to perform identification processes. The classification model is constructed according to the personal history and the pre-trained parameters. Thereby, the present invention can obtain the analysis result corresponding to the abovementioned brain electrical signal, i.e. the status of brain activity. After obtaining the status of brain activity, the signal processing unit 12 presents the result on the display unit 16.

[0021] Succeeding to full demonstration of the spirit of the present invention, the example shown in Fig. 4(a) and Fig. 4(b) is used to illustrate the technical contents of the present invention. The encircled portions are the features selected by the feature mask $M = x(\text{FM}[2], \text{AM}[1(\text{FM}[1,2], \text{AM}[1,2]), 2])$, wherein x denotes the brain electrical signal; the Arabic numerals 1, 2 denotes the sub-signals; AM denotes amplitude modulation; FM denotes frequency modulation. Fig. 4(a) shows the brain electrical signal detected in seizure. The signal in Fig. 4(a) is decomposed into a plurality of intrinsic feature sub-signals in a nonstationary decomposition method, as shown in Fig. 4(b). Each of the sub-signals in Fig. 4(b) is demodulated into a frequency-modulation part and an amplitude-modulation part, as shown in Fig. 4(c). The modulation signals $x(\text{FM}[2])$ and $x(\text{AM}[1,2])$ are selected as the features to be used in the succeeding calculation. The modulation signal $x(\text{AM}[1])$ is further decomposed

- using said feature mask to select said modulation signals of interest as feature modulation signals from all said modulation signals; and performing quantitation processes and identification processes of said feature modulation signals to obtain an analysis result corresponding to said brain electrical signal.
2. The brain activity analysis method according to claim 1, wherein said brain electrical signal is obtained via using a sensing unit to measure brain waves of at least one subject.
 3. The brain activity analysis method according to claim 1, wherein said brain electrical signal is an electroencephalography (EEG) signal, an intracranial electroencephalogram (iEEG) signal, or an electrocorticography (ECoG) signal.
 4. The brain activity analysis method according to claim 1, wherein said nonstationary decomposition method is an empirical mode decomposition (EMD) method.
 5. The brain activity analysis method according to claim 1, wherein in said step of demodulating each of said sub-signals, a normalization operation is used to demodulate each of said sub-signals into said modulation signals.
 6. The brain activity analysis method according to claim 1, wherein said modulation signals include frequency-modulation parts and amplitude-modulation parts.
 7. The brain activity analysis method according to claim 1, wherein said feature mask is in form of a word string, a sequence matrix or a multidimensional matrix.
 8. The brain activity analysis method according to claim 1, wherein said analysis result is a status of brain activity.
 9. The brain activity analysis method according to claim 1, wherein said quantitation processes include calculation of power densities, instantaneous frequencies, or averaged periods.
 10. The brain activity analysis method according to claim 1, wherein a classification model is used in said identification processes, and wherein said classification model involves personal history and pre-trained parameters.
 11. A brain activity analysis apparatus, which processes at least one brain electrical signal to generate an analysis result, comprising
 - at least one sensing unit detecting brain waves of a subject to acquire said at least one brain electrical signal;
 - a signal processing unit being in communication with said sensing unit to receive said brain electrical signal, using a nonstationary decomposition method to decompose said brain electrical signal to acquire a plurality of sub-signals carrying intrinsic feature components, demodulating each of said sub-signals to generate modulation signals respectively corresponding to said sub-signals, undertaking recursive iteration of said modulation signals, selecting said modulation signals of interest from all said modulation signals as feature modulation signals, and undertaking quantitation processes and identification processes of said feature modulation signals to obtain an analysis result corresponding to said brain electrical signal; and
 - a display unit electrically connected with said signal processing unit and presenting said analysis result.
 12. The brain activity analysis apparatus according to claim 11, wherein said brain electrical signal is an electroencephalography (EEG) signal, an intracranial electroencephalogram (iEEG) signal, or an electrocorticography (ECoG) signal.
 13. The brain activity analysis apparatus according to claim 11, wherein said nonstationary decomposition method is an empirical mode decomposition (EMD) method.
 14. The brain activity analysis apparatus according to claim 11, wherein a normalization operation is used to demodulate each of said sub-signals to obtain said modulation signals.
 15. The brain activity analysis apparatus according to claim 11, wherein said modulation signals include frequency-modulation parts and amplitude-modulation parts.
 16. The brain activity analysis apparatus according to claim 11, wherein said analysis result is a status of brain activity.
 17. The brain activity analysis apparatus according to claim 11, wherein said quantitation processes include calculation of power densities, instantaneous frequencies, or averaged periods.
 18. The brain activity analysis apparatus according to claim 11, wherein a classification model is used in said identification processes, and wherein said classification model involves personal history and pre-trained parameters.

19. The brain activity analysis apparatus according to claim 11 further comprising a storage unit electrically connected with said signal processing unit for storing signals, data and results processed by said signal processing unit.

5

20. The brain activity analysis apparatus according to claim 11, wherein said feature mask is in form of a word string, a sequence matrix or a multidimensional matrix.

10

15

20

25

30

35

40

45

50

55

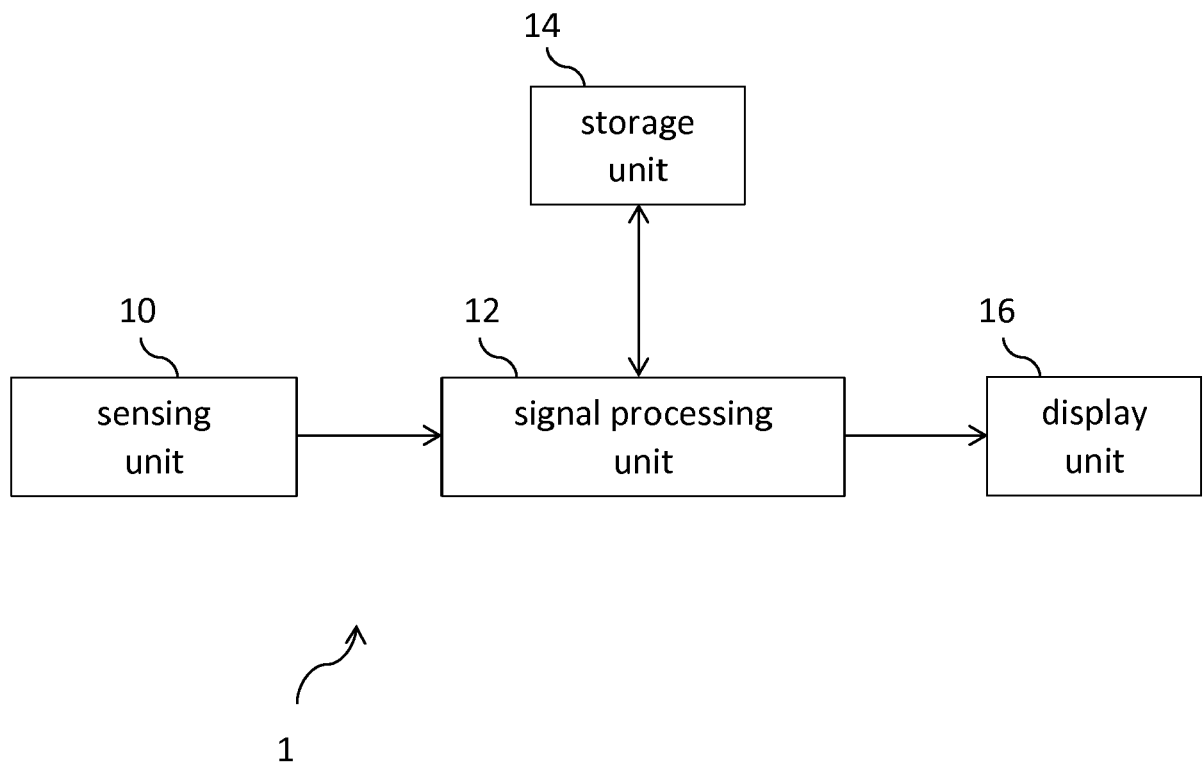


FIG.1

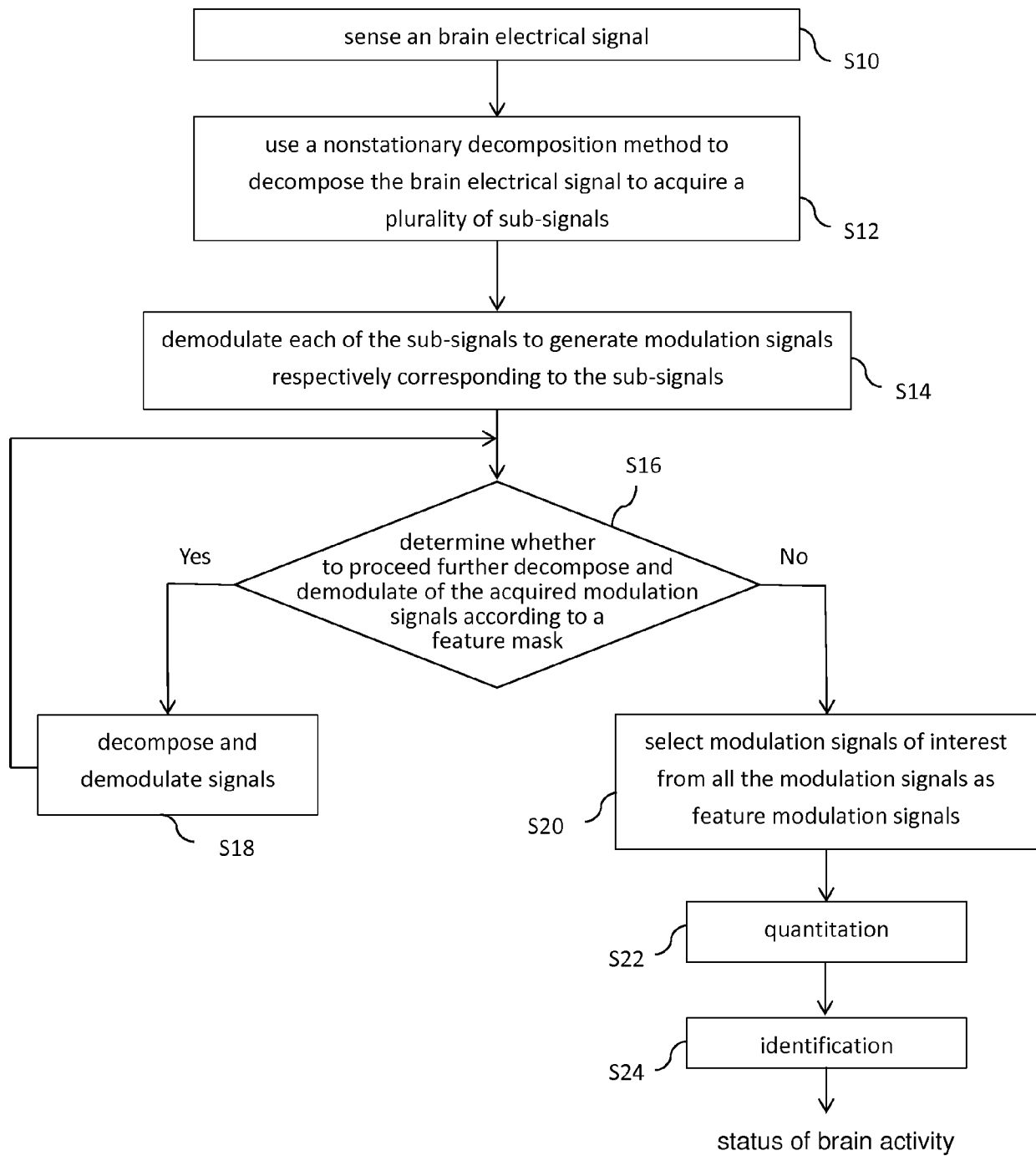


FIG.2

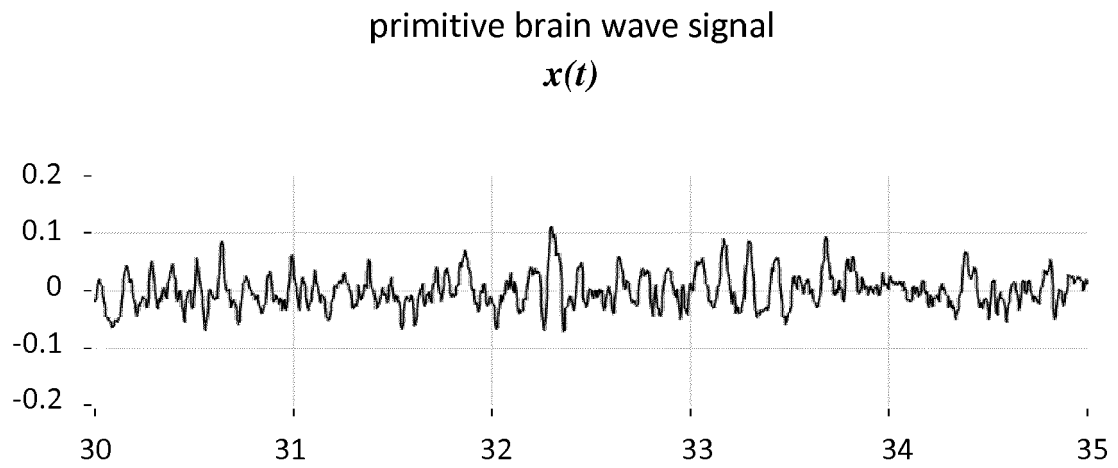


FIG.3(a)

sub-signals with intrinsic feature

$$\Sigma A_i(t) e^{jw_i(t)t}$$

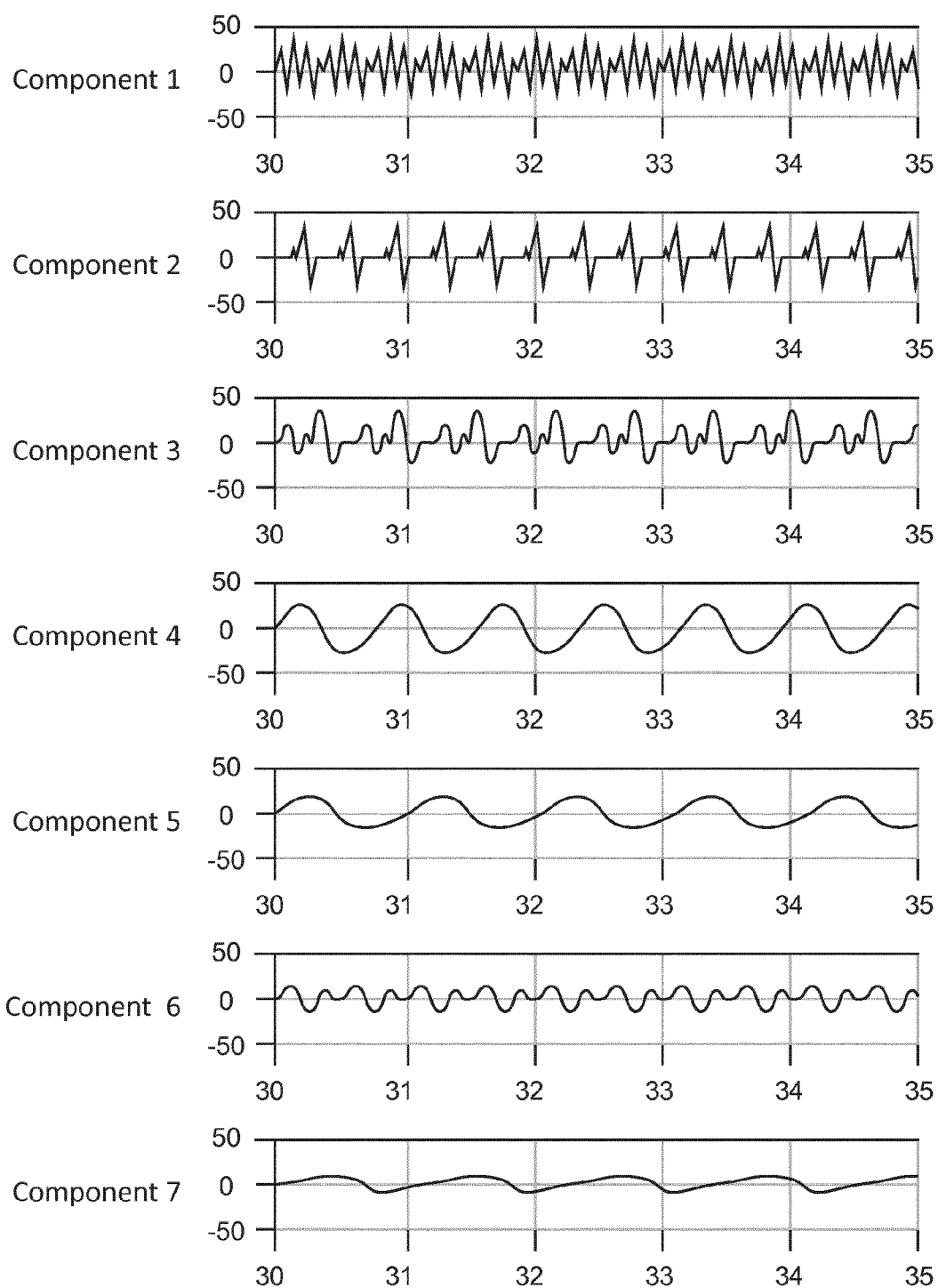


FIG.3(b)

frequency-modulation parts

amplitude-modulation parts

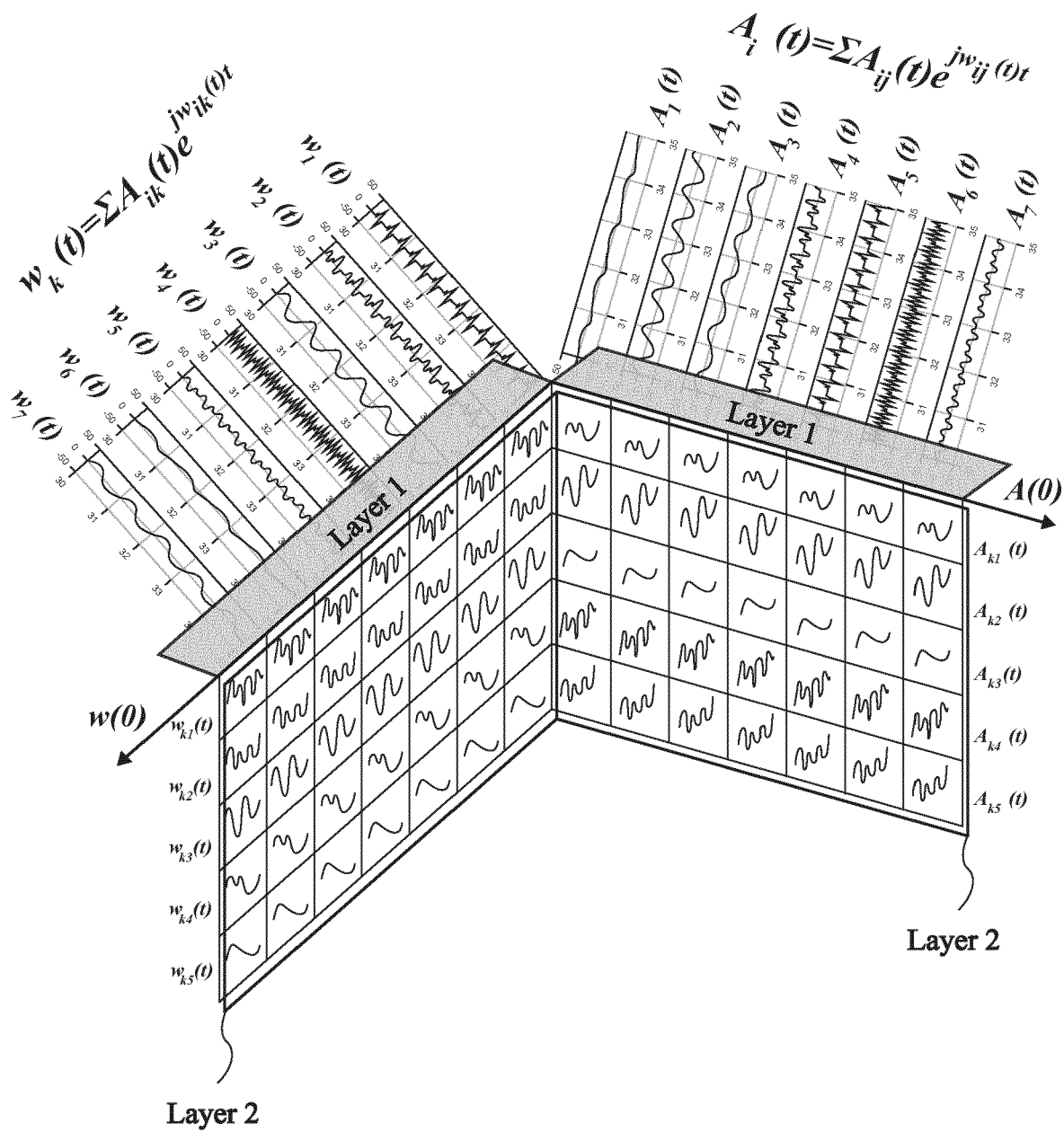


FIG.3(c)

frequency-modulation parts

amplitude-modulation parts

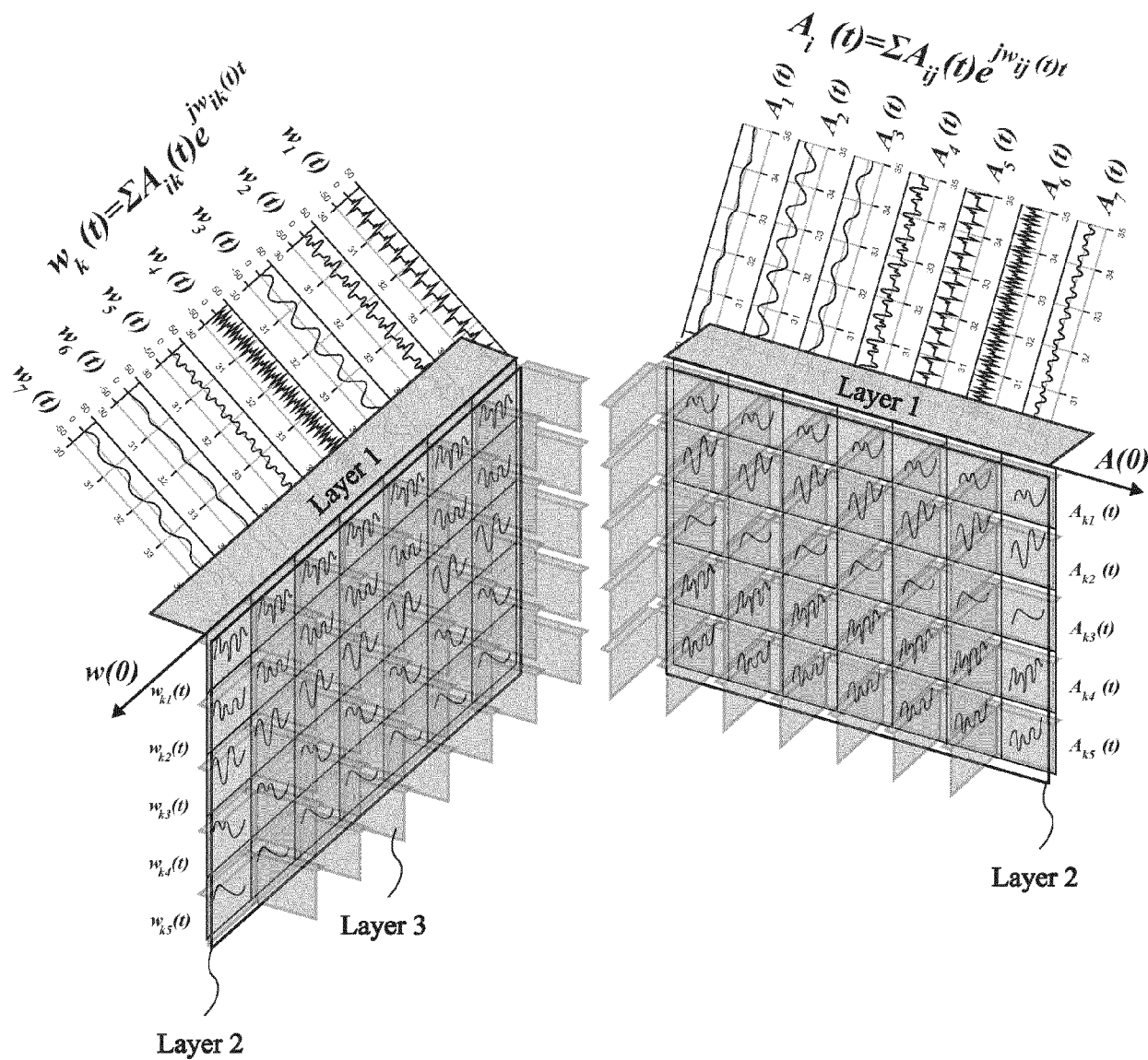


FIG.3(d)

frequency-modulation parts

amplitude-modulation parts

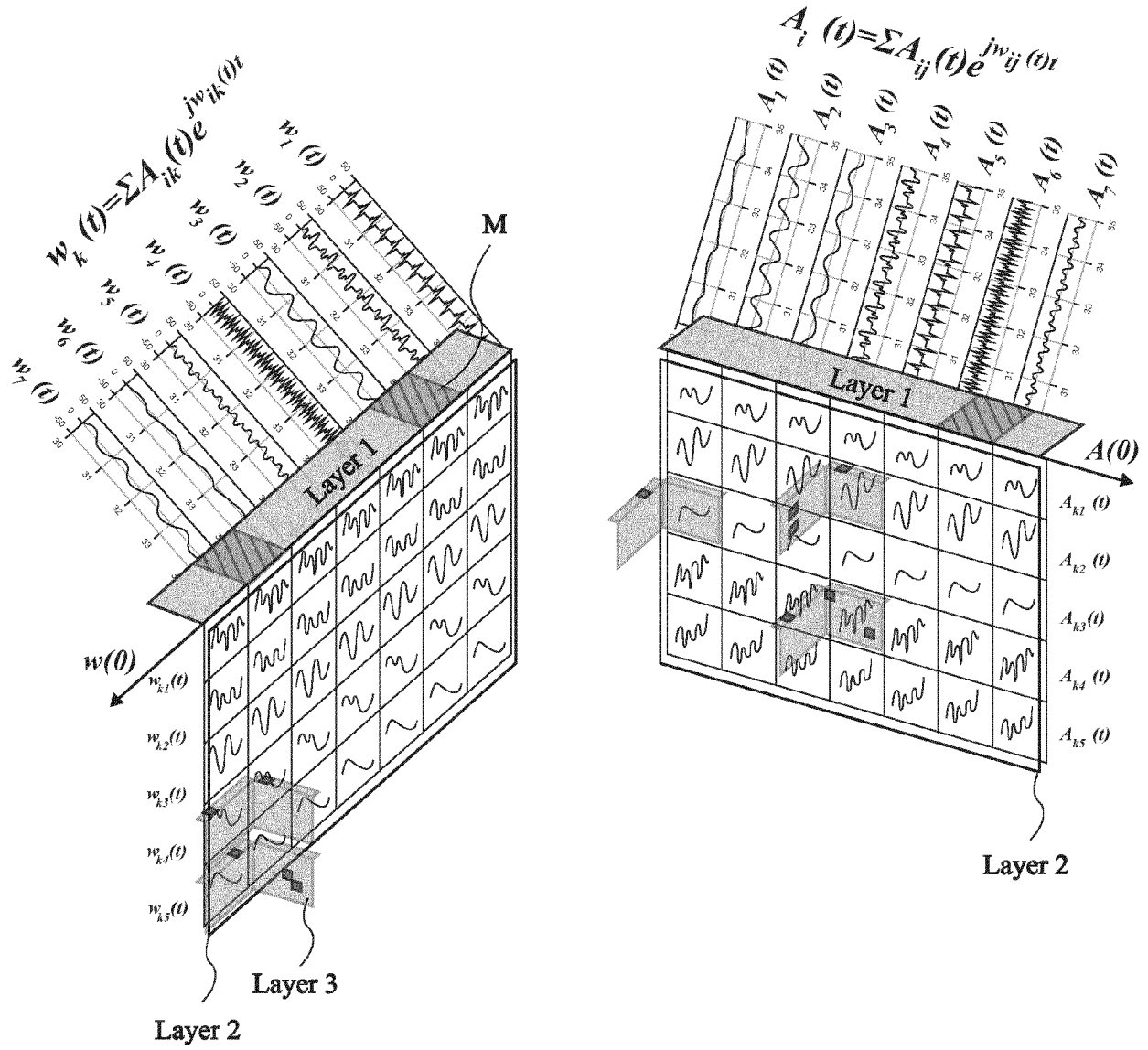


FIG.3(e)

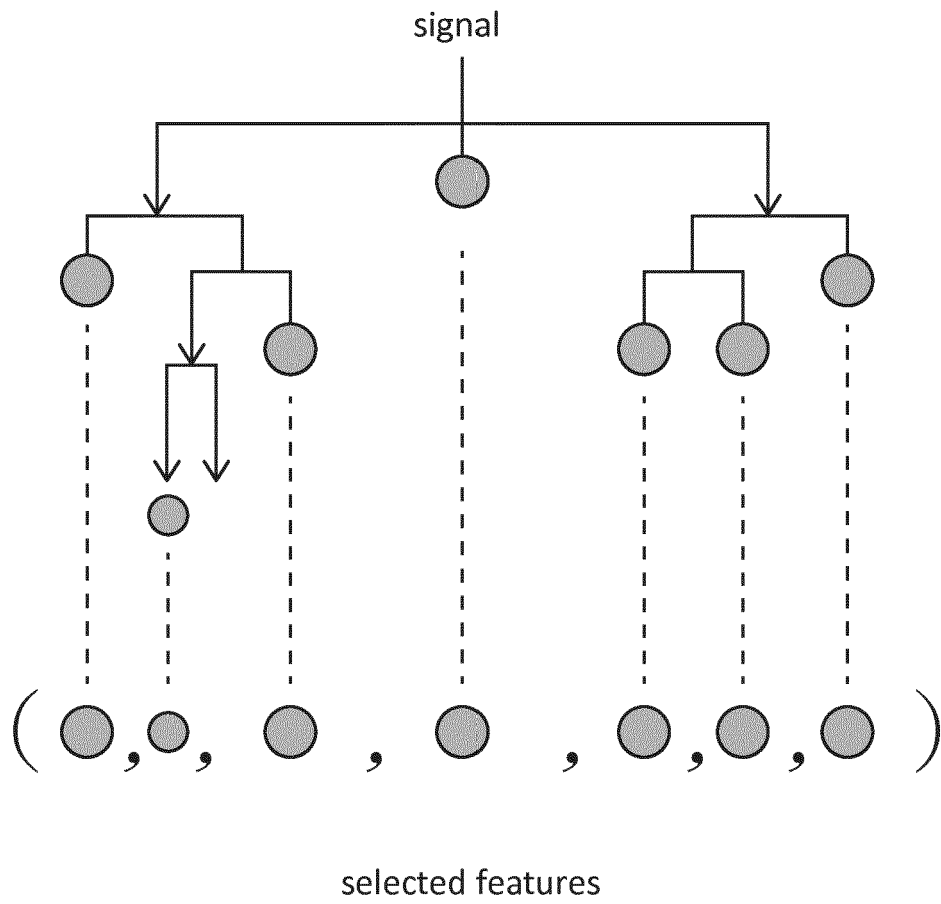


FIG.3(f)

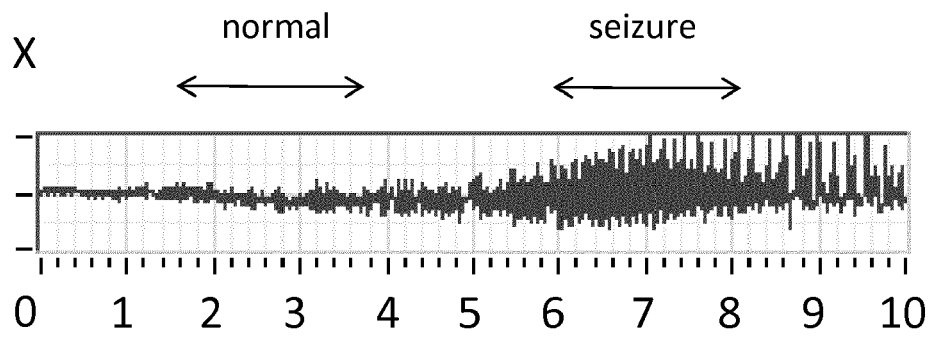


FIG.4(a)

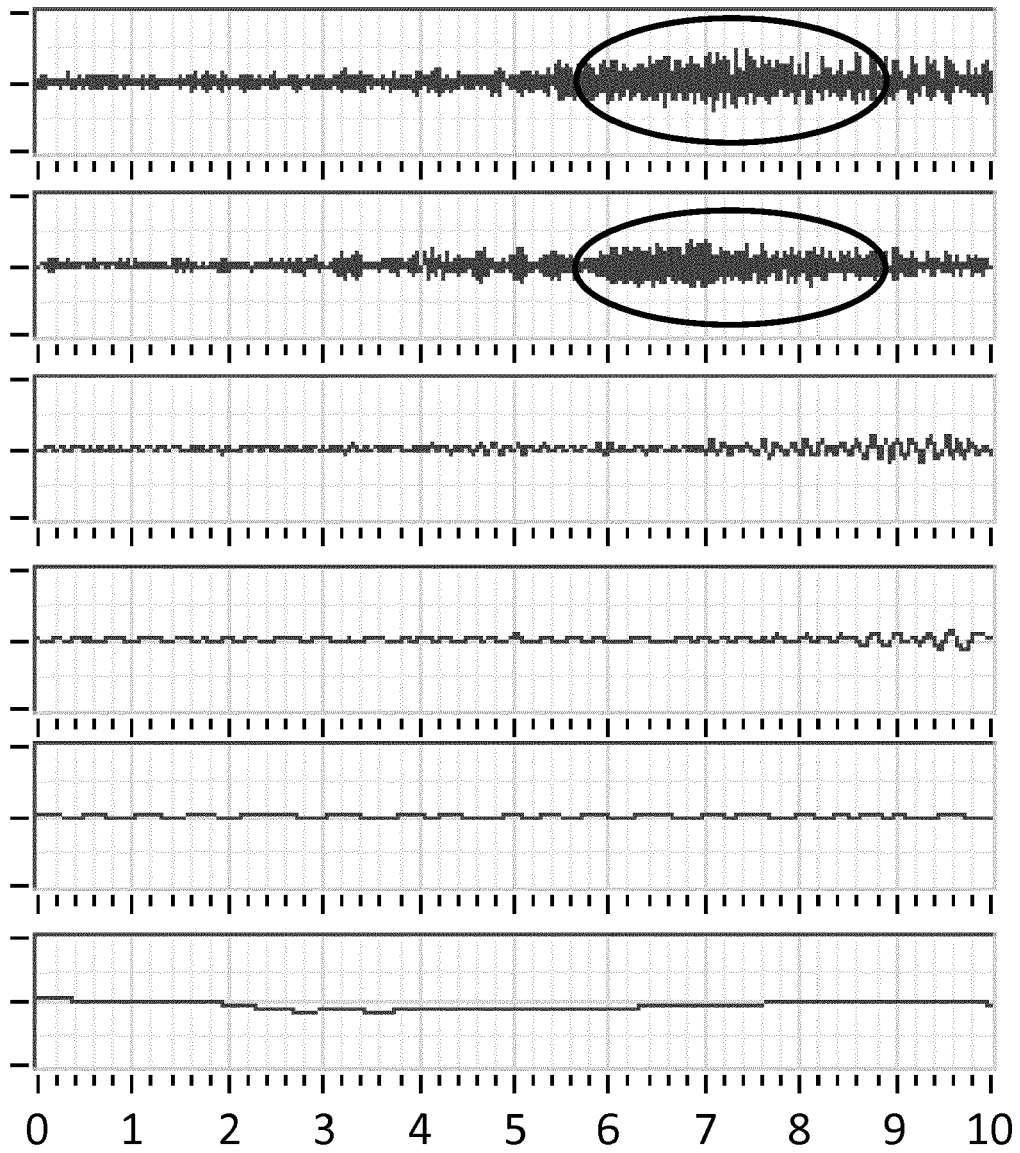


FIG.4(b)

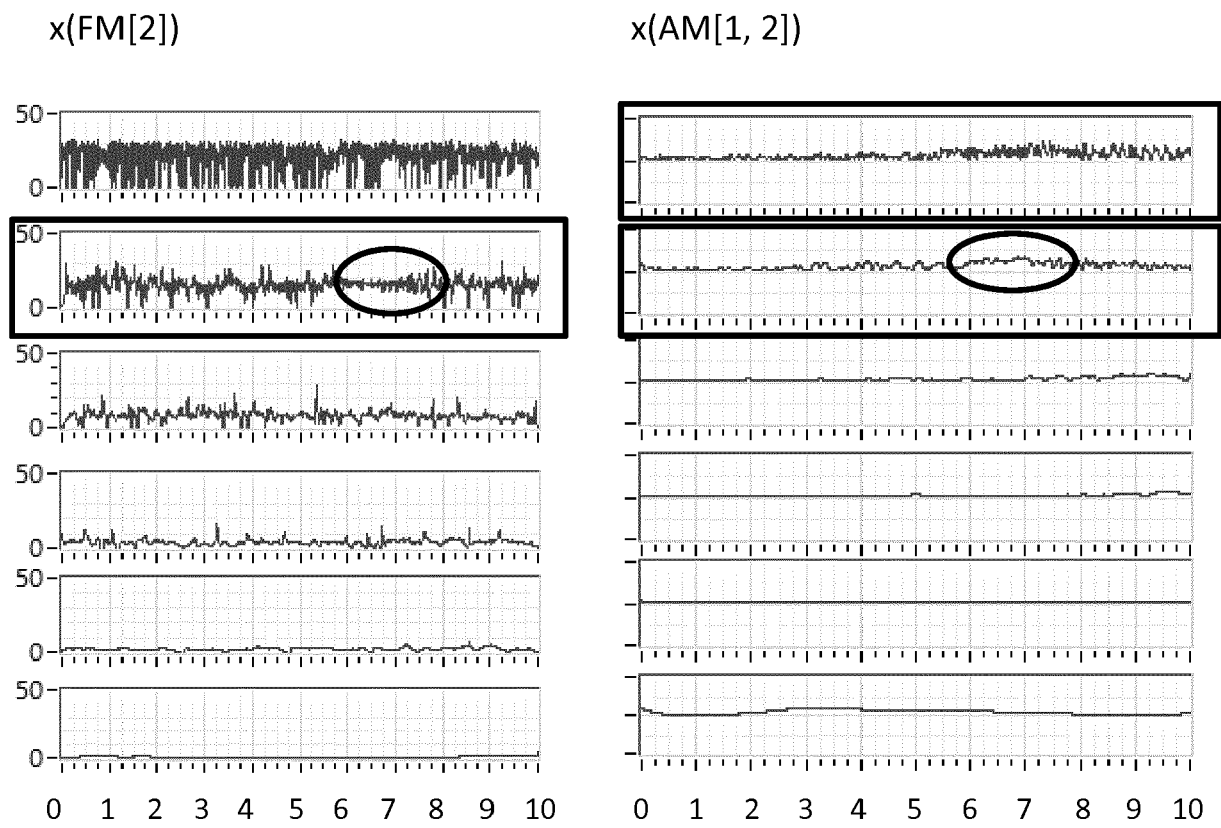


FIG.4(c)

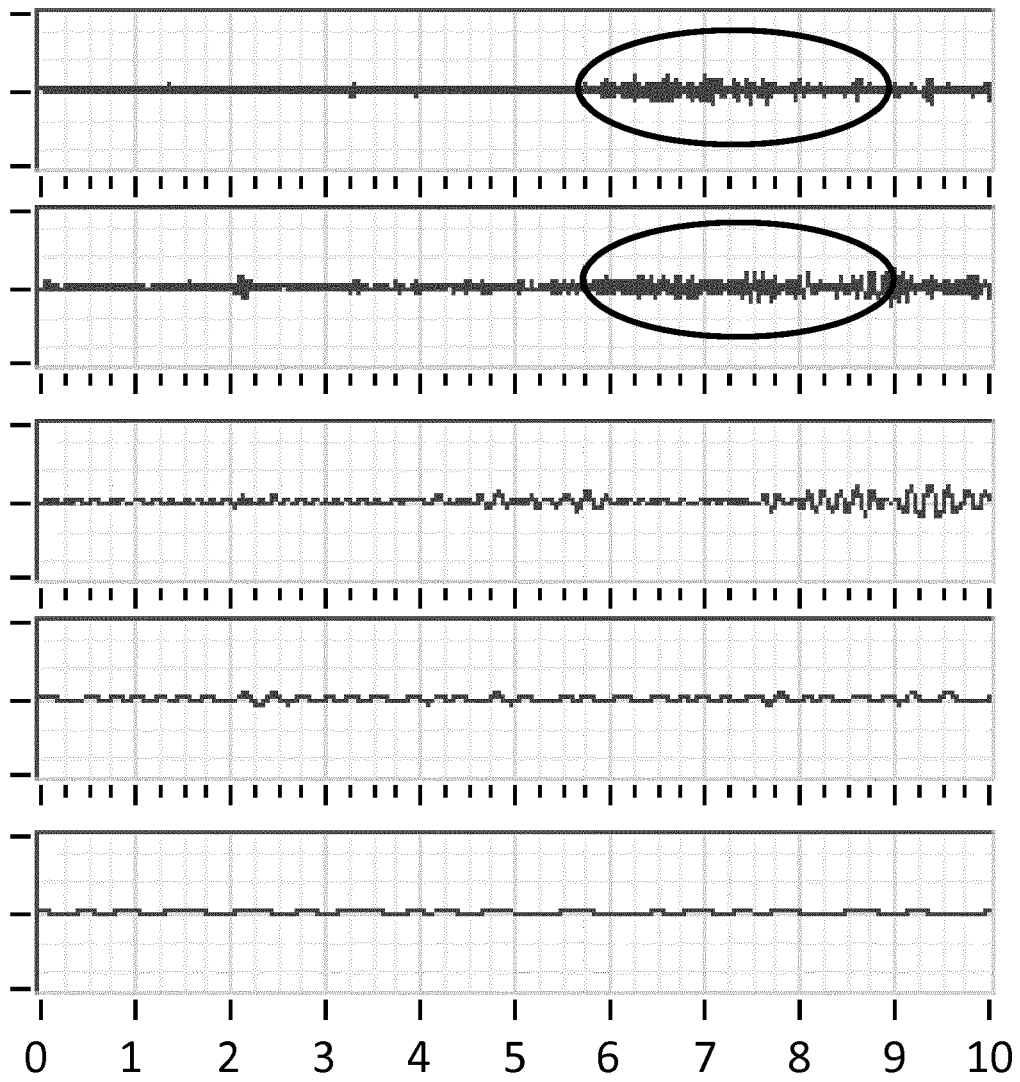
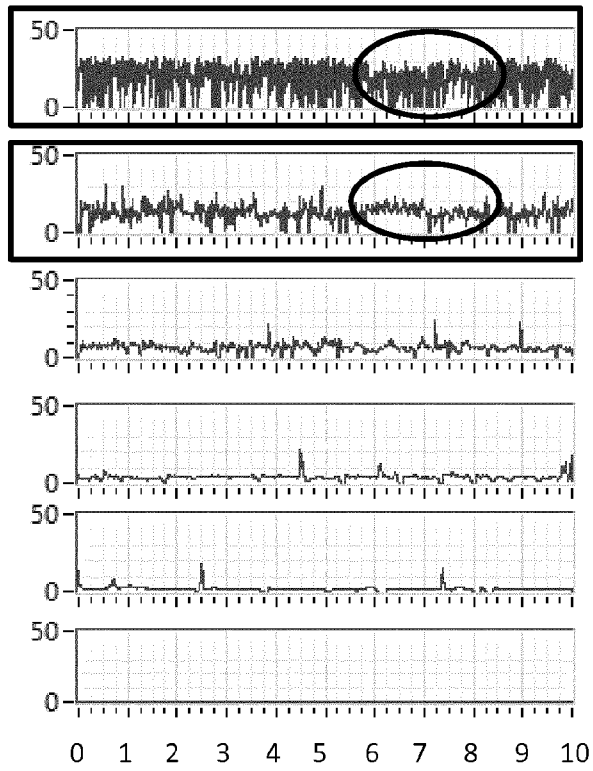


FIG.4(d)

$x(\text{AM}[1(\text{FM}[1, 2])])$



$x(\text{AM}[1(\text{AM}[1, 2])])$

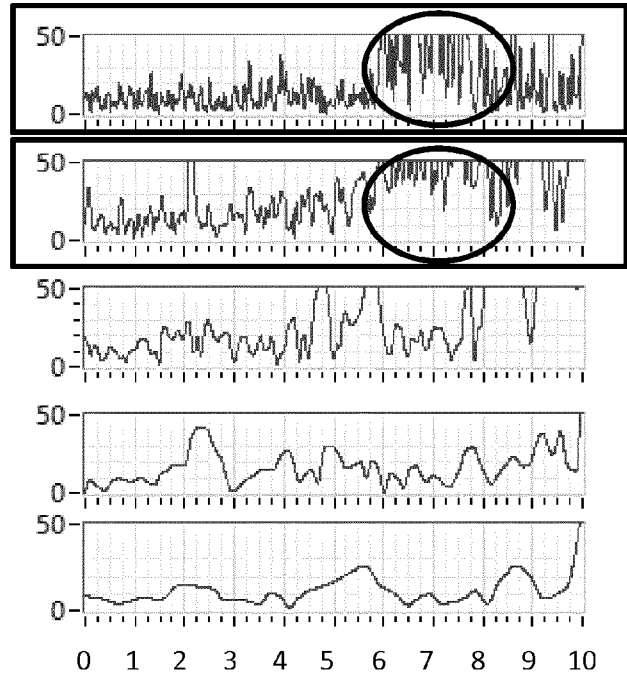


FIG.4(e)



EUROPEAN SEARCH REPORT

Application Number
EP 17 17 5004

5

10

15

20

25

30

35

40

45

50

55

DOCUMENTS CONSIDERED TO BE RELEVANT			
Category	Citation of document with indication, where appropriate, of relevant passages	Relevant to claim	CLASSIFICATION OF THE APPLICATION (IPC)
A	US 2006/111644 A1 (GUTTAG JOHN V [US] ET AL) 25 May 2006 (2006-05-25) * paragraphs [0242], [0243] * -----	1-20	INV. A61B5/00 A61B5/0476 A61B5/048 G16H50/20
A	CN 102 824 173 B (BEIJING INST TECHNOLOGY) 2 April 2014 (2014-04-02) * abstract * -----	1-20	
A	MARK G. FREI ET AL: "Intrinsic time-scale decomposition: time-frequency-energy analysis and real-time filtering of non-stationary signals", PROCEEDINGS - ROYAL SOCIETY. MATHEMATICAL, PHYSICAL AND ENGINEERING SCIENCES, vol. 463, no. 2078, 15 August 2006 (2006-08-15), pages 321-342, XP055033558, ISSN: 1364-5021, DOI: 10.1098/rspa.2006.1761 * the whole document * -----	1-20	
			TECHNICAL FIELDS SEARCHED (IPC)
			A61B G16H
The present search report has been drawn up for all claims			
Place of search Berlin		Date of completion of the search 7 March 2018	Examiner Pohjamo, Terhi
CATEGORY OF CITED DOCUMENTS X : particularly relevant if taken alone Y : particularly relevant if combined with another document of the same category A : technological background O : non-written disclosure P : intermediate document T : theory or principle underlying the invention E : earlier patent document, but published on, or after the filing date D : document cited in the application L : document cited for other reasons & : member of the same patent family, corresponding document			

EPO FORM 1503 03/02 (P04C01)

**ANNEX TO THE EUROPEAN SEARCH REPORT
ON EUROPEAN PATENT APPLICATION NO.**

EP 17 17 5004

5

This annex lists the patent family members relating to the patent documents cited in the above-mentioned European search report.
The members are as contained in the European Patent Office EDP file on
The European Patent Office is in no way liable for these particulars which are merely given for the purpose of information.

07-03-2018

10

Patent document cited in search report	Publication date	Patent family member(s)	Publication date
US 2006111644 A1	25-05-2006	US 2006111644 A1	25-05-2006
		US 2011257517 A1	20-10-2011
		WO 2005117693 A1	15-12-2005

CN 102824173 B	02-04-2014	NONE	

15

20

25

30

35

40

45

50

55

EPO FORM P0459

For more details about this annex : see Official Journal of the European Patent Office, No. 12/82

REFERENCES CITED IN THE DESCRIPTION

This list of references cited by the applicant is for the reader's convenience only. It does not form part of the European patent document. Even though great care has been taken in compiling the references, errors or omissions cannot be excluded and the EPO disclaims all liability in this regard.

Patent documents cited in the description

- TW 106114720 [0001]
- US 6480743 B [0005]
- US 8131352 B [0005]
- US 6810285 B [0005]
- TW I487503 [0005]

专利名称(译)	脑活动分析方法和装置		
公开(公告)号	EP3398505A1	公开(公告)日	2018-11-07
申请号	EP2017175004	申请日	2017-06-08
[标]发明人	CHANG CHIA CHI LIN PEI CHEN		
发明人	CHANG, CHIA-CHI LIN, PEI-CHEN		
IPC分类号	A61B5/00 A61B5/0476 A61B5/048 G16H50/20		
CPC分类号	A61B5/04012 A61B5/0476 A61B5/7235 A61B5/7264 A61B5/048 A61B5/4094 A61B5/7282 G16H40/63 G16H50/20 A61B5/7228 A61B5/742		
代理机构(译)	LANG , CHRISTIAN		
优先权	106114720 2017-05-04 TW		
外部链接	Espacenet		

摘要(译)

本发明公开了一种脑活动分析方法和装置，其基于非线性波形分解技术，其中脑波中固有特征的变化被分解和解调，以提取组件的调制信号，包括调频信号。和幅度调制信号。它还使用特征掩码来确定是否进一步分解和解调所提取的调制信号。如果不是，则根据特征掩模获得固有特征的多维变化。然后，进行定量和鉴定以获得脑功能的状态。它不仅有效地提高了识别的准确性，而且还使用特征掩码来明显降低计算的复杂性和负担。

