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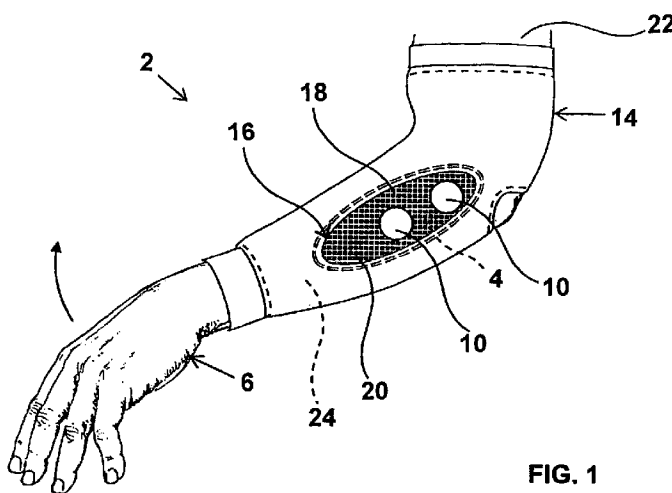


FIG. 1

(57) Abstract: Apparatus (2) for providing information on at least one muscle (4) in a patient (6), which apparatus (2) comprises: (i) signal providing means (8) for providing measurement-enabling signals for the muscle (4); (ii) first contact electrodes (10) for enabling the measurement-enabling signals from the signal providing means to be received by the patient (6); (iii) measurement means (12) for measuring a parameter of the muscle (4), the parameter being such that it is affected by the measurement-enabling signals, and the parameter being such that it relates to at least one electrical property that is indicative of changes in tissue impedance caused by movement of the muscle (4); and (iv) a garment (14) which is for being worn over the muscle (4) in the patient (6) and which comprises an array (16) of separate electrically conducting areas (18), and the apparatus (2) being such that the first contact electrodes (10) are able to be positioned on the garment (14) at a predetermined precise position for obtaining the measured parameter and with the first contact electrodes (10) being in contact with those separate electrically conducting areas in the garment (14) that are over the predetermined position. The apparatus optionally includes neuromuscular stimulator means (46) for providing neuromuscular stimulation signals for the muscle (4).



APPARATUS FOR USE FOR PROVIDING INFORMATION
ON AT LEAST ONE MUSCLE IN A PATIENT

This invention relates to apparatus for providing information on at least one muscle in a patient. The apparatus may be for providing information on the movement of the muscle in a patient suffering loss of mobility due to illness caused for example by a stroke or surgery. The apparatus may also be used for providing information on the movement of the muscle in a patient who is able bodied but who wishes to achieve better performance with better muscle movement, for example in the case of athletes. The apparatus of the present invention is primarily for use for human patients but it may also be used for animal patients.

Known apparatus for providing information on at least one muscle in a patient comprises signal providing means for providing measurement-enabling signals for the muscle, contact electrodes for enabling the measurement-enabling signals from the signal providing means to be received by the patient, and measurement means for measuring a parameter of the muscle. The known apparatus is used for giving an indication of joint articulation, for example ankle articulation. A problem with the known apparatus is that it is difficult to position the contact electrodes precisely on the required part of the patient. Variations in positioning of plus or minus 5mm from an optimum position may adversely affect measurement results.

It is an aim of the present invention to reduce the above mentioned problem.

Accordingly, in one non-limiting embodiment of the present invention there is provided apparatus for providing information on at least one muscle in a patient, which apparatus comprises:

- (i) signal providing means for providing measurement-enabling signals for the muscle;
- (ii) first contact electrodes for enabling the measurement-enabling signals from the signal providing means to be received by the patient;
- (iii) measurement means for measuring a parameter of the muscle, the parameter being such that it is affected by the measurement-enabling signals, and the parameter being such that it relates to at least one electrical property that is indicative of changes in tissue impedance cause by movement of the muscle; and
- (iv) a garment which is for being worn over the muscle in the patient and which comprises an array of separate electrically conducting areas,

and the apparatus being such that the first contact electrodes are able to be positioned on the garment at a predetermined precise position for

obtaining the measured parameter and with the first contact electrodes being in contact with those separate electrically conducting areas in the garment that are over the predetermined position.

The apparatus of the present invention is advantageous in that it enables the precise positioning of the first contact electrodes. This precise positioning is achievable for individual patients. Once the precise position of the first contact electrodes on the garment has been established, then the first contact electrodes are able to be secured in position on the garment, for example using securing means such for example as an adhesive. The adhesive may be an electrically conductive gel which allows adjustment repositioning of the contact electrodes prior to the electrically conductive gel curing. The initial precise positioning of the first contact electrodes on the garment may be effected by a clinician, hospital technician or other authorised person. Once the first electrodes have been secured to the garment, the garment can then be taken off after use and later put on as necessary, for example for daily use. The patient may be the person that puts the garment on and takes it off. The repeated precise positioning of the first contact electrodes is assured because they are secured to the garment. Reliable remote monitoring of the patient's muscle movement, for example from another part of the hospital or from home thus becomes possible.

The apparatus may be one in which the garment is made of a fabric which is stretchable or conformal. A garment made of such a fabric enables

the garment to conform to the part of the patient's body requiring measurement of the muscle in order to indicate the movement of the muscle.

The garment may be a sleeve garment for being slid over a part of the patient. The part of the patient may be, for example an arm, a leg, a finger, a toe, a torso or a neck. The sleeve garment may be a closed loop sleeve garment which stretches in order to be placed over the part of the person.

If desired, the garment may be a strap garment for being strapped around a part of the patient. The strap garment may be in the form of an open loop which is closed by closure means. The closure means may be a fastener comprising a matrix of push to close and pull to open plastics members. One such preferred type of fastener is that known under the Registered Trade Mark Velcro. Other closure means may be employed, for example a buckle.

The array of separate electrically conducting areas may be separated by non-electrically conducting areas, or by lower electrically conducting areas. Preferably, the lower electrically conducting areas are thinner than the electrically conducting areas in order to limit current flow laterally. Usually, the electrically conducting areas in the array will be spaced apart from each other. Other types of electrically conducting areas may however be employed. The electrically conducting areas may be such that they conduct transversely through the garment but not, or not substantially, in the plane of the garment. Thus the electrically conducting areas may be regarded as being trans-conductive electrically conducting areas.

The electrically conducting areas may be woven into the garment or they may be moulded or printed into the garment.

The array may be any suitable and appropriate size and shape. Thus, for example, the array may be of a regular or irregular shape dependent upon the position and size of a muscle or muscle group being monitored or treated.

The apparatus of the present invention may be used to provide a measured parameter that only indicates movement of the muscle. The signal providing means may be a separate signal generator. There will usually be two of the first contact electrodes but more than two of the first contact electrodes may be employed if desired.

Alternatively, in addition to providing a measured parameter that indicates movement of the muscle, the apparatus of the present invention may also be used to provide neuromuscular stimulation of the muscle as determined by the indicated movement of the muscle. In this case, the apparatus of the present invention may include neuromuscular stimulator means for providing neuromuscular stimulation signals for the muscle.

When the apparatus of the present invention includes the neuromuscular stimulator means, then the signal providing means and the neuromuscular stimulator means may be provided as a single component. Alternatively, the signal providing means may be provided as a separate component from the neuromuscular stimulator means.

When the apparatus of the present invention includes the neuromuscular stimulator means, then the apparatus may be used such that the measurement-enabling signals for the muscle are imposed on the neuromuscular stimulation signals for the muscle, or vice versa.

If desired, the first contact electrodes may also enable the neuromuscular stimulation signals to be received by the patient. Alternatively, the apparatus of the present invention may include second contact electrodes which are separate from the first contact electrodes and which enable the neuromuscular stimulation signals to be received by the patient, the second contact electrodes being able to be positioned on the garment in a predetermined position for obtaining the neuromuscular stimulation and with the second contact electrodes being in contact with those separately electrically conducting areas in the garment that are over the predetermined position. When second contact electrodes are employed, there will usually be two of the second contact electrodes but more than two of the second contact electrodes may be employed if desired.

The measurement-enabling signals may have a waveform selected from at least one of:

- (a) a sine wave;
- (b) a square wave;
- (c) a triangular wave;
- (d) an arbitrary wave form shape;
- (e) repeated parts of similar or dissimilar wave forms;
- (f) a random wave form capable of being averaged; and
- (g) an impulse.

Other types of wave forms may be employed. The random wave form may be a wave form that has noise properties, for example white noise.

The measurement means may be such that it measures the parameter of the muscle by using an electrical property selected from at least one of:

- (a) phase shift;
- (b) amplitude;
- (c) slew rate;
- (d) a root mean squared value; and
- (e) impulse.

Other electrical properties may be measured if desired.

The apparatus of the present invention may include sealing means for sealing electronically conducting parts on the garment, whereby the garment is able to be cleaned. Thus, for example, after repeated use the garment may be cleaned by sponging.

The apparatus of the present invention may be used such that a clinician or other person will accurately position the first contact electrodes onto the most appropriate area of the array of separately conducting areas. The first contact electrodes may remain in place for all future uses of the garment. Alternatively, the first electrodes may be removable after a use and then be repositionable for each subsequent use. When the first electrodes are to remain in place, they may be constructed for connection to the remainder of the apparatus.

The apparatus of the present invention may be used such that the movement of the muscle is a movement caused by changes to muscle length. Other types of muscle movement may however be used.

Embodiments of the invention will now be described solely by way of example and with reference to the accompanying drawings in which:

Figure 1 shows part of first apparatus for providing information on at least one muscle in a patient, and for ensuring accurate and repeatable location of electrodes;

Figure 2 is an enlarged view of part of the apparatus shown in Figure 1;

Figure 3 is a cross section through a part of the apparatus shown in Figure 1;

Figure 4 is an enlarged view of part of the apparatus shown in Figure 3;

Figures 5 – 10 show different types of separate electrically conducting areas to those shown in Figure 1;

Figure 11 shows part of first apparatus of the present invention which provides a measured parameter that indicates the movement of the muscle;

Figure 12 shows part of second apparatus of the present invention including measurement means for indicating movement of a muscle and also neuromuscular stimulator means for providing neuromuscular stimulation signals for the muscle;

Figure 13 shows part of third apparatus of the present invention wherein both signal providing means for providing measurement-enabling

signals for the muscle and neuromuscular stimulation signals for the muscles are provided by a neuromuscular stimulator;

Figure 14 shows part of fourth apparatus of the present invention, the apparatus comprising a first set of electrodes for enabling the measurement-enabling signals from the signal providing means to be received by a patient, and a second set of electrodes for receiving neuromuscular stimulation signals from neuromuscular stimulator means;

Figure 15 shows a measurement wave form for use with a separate signal generator and neuromuscular stimulator as shown in the apparatus of Figures 12 and 14; and

Figure 16 shows a measurement wave form using a component of a neuromuscular stimulation wave as a measurement-enabling signal, as shown in the apparatus of Figure 13.

Referring to Figures 1 – 4 and 11 there is shown apparatus 2 for use for at least one muscle 4 in a patient 6. The apparatus 2 comprises signal providing means 8 for providing measurement-enabling signals for the muscle 4. The apparatus 2 also comprises two first contact electrodes 10 for enabling the measurement-enabling signals from the signal providing means 8 to be received by the patient 6.

The apparatus 2 further comprises measurement means 12 for measuring a parameter of the muscle 4. The parameter is such that it is affected by the measurement-enabling signals. The parameter is such that it relates to at least one electrical property that is indicative of changes in tissue impedance caused by movement of the muscle 4.

The apparatus 2 further comprises a garment 14 which is for being worn over the muscle 4 in the patient 6. The garment 14 comprises an array 16 of separate electrically conducting areas 18 separated by non-electrically conducting areas 20.

The apparatus 2 is such that the first contact electrodes 10 are able to be positioned on the garment 14 at a predetermined precise position for obtaining the measured parameter, and with the first contact electrodes 10 being in contact with those separate electrically conducting areas 18 in the garment 14 that are over the predetermined position.

As shown in Figure 1, the garment is a sleeve garment which is slid over an arm 22 such that the garment 14 is on a forearm 24 of the arm 22. The garment 14 is made of a fabric which is stretchable or conformable whereby the garment 14 is a sleeve garment which conforms closely to the contours of the forearm 24.

Figure 3 shows how the matrix 16 of the electrically conducting areas 18 is able to be in contact with the skin 25 of the patient 6.

The separate electrically conducting areas 18 are regularly spaced separate electrically conducting areas 18 in the array 16. The separate electrically conducting areas 18 are woven into the garment or are moulded or printed into the garment, as can best be appreciated from Figures 3 and 4.

Figures 5 – 10 show six different types and/or configurations of separate electrically conducting areas 18 and surrounding non-electrically conducting areas 20 in arrays 26, 28, 30, 32, 34, 36.

Figure 11 shows how the first apparatus 2 is such that the signal providing means 8 is a separate signal generator. In use, the signal generator 8 produces a measurement wave form 38 that creates an electrical circuit 40 through the patient's body via the first contact electrodes 10, the electrically conducting areas 18 and the measurement means 12. The measurement means 12 produces an output 42. The output 42 is thus a measured parameter that indicates movement of the muscle 4.

Figure 12 shows part of second apparatus 44 of the present invention. Similar parts as in Figure 11 have been given the same reference numerals for ease of comparison and understanding. The apparatus 44 is such that it includes neuromuscular stimulator means 46 for providing neuromuscular stimulating signals for the muscle 4. The use of the neuromuscular stimulator means is additional to the use of the signal providing means 8 as will be appreciated from Figure 12. Thus the apparatus 44 enables the muscle 4 firstly to be measured in order to obtain an indication of the movement of the muscle 4, and secondly to receive neuromuscular stimulation signals for stimulating movement of the muscle 4. The effect of the neuromuscular stimulation can then be monitored by the measured parameter indicating the movement of the muscle 4 and the neuromuscular stimulation signals can then be adjusted accordingly for providing optimum neuromuscular stimulation for the muscle 4. The apparatus 44 operates such that the signal providing means 8 produces the wave form 38. The wave form 38 is switched by a switch 48 to form the electrical circuit 40 through the patient's body via the electrodes 10 and the measurement means 12. The calculation is made

by the measurement means 12, and a control command signal 50 is then sent to the neuromuscular stimulator means 46. The neuromuscular stimulator means 46 is connected to the first contact electrodes 10 via the switch 48, and thus a stimulation pulse or pulses 52 are delivered to the first contact electrodes 10. The process is then repeated as necessary and appropriate.

Figure 13 shows third apparatus 54. Similar parts as in previous Figures have been given the same reference numerals for ease of comparison and understanding. In operation of the apparatus 54, the neuromuscular stimulator means 46 produces a neuromuscular stimulation pulse train 52 which is delivered to the first contact electrodes 10. An electrical circuit 40 is formed through the measurement means 12. The measurement means 12 calculates a control signal 50 which is sent to the neuromuscular stimulator means 46 to modulate the pulse train 52. The measurement-enabling signals are formed as a component of the neuromuscular stimulation pulse train 52. The measurement-enabling signals are generated by signal providing means 8 which are not shown in Figure 13 but which are formed as an integral part of the neuromuscular stimulator means 46.

Figure 14 shows fourth apparatus 56 of the present invention. Similar parts as in previous Figures have been given the same reference numerals for ease of comparison and understanding. The apparatus 56 is like the apparatus 44 except that the apparatus 56 employs the first contact electrodes 10 and also two second contact electrodes 58. This enables the apparatus 56 to dispense with the switch 48 used in the apparatus 44. The

apparatus 56 operates such that the signal providing means 8 produces a measurement wave form 38 to form an electrical circuit 40 through the body of the patient 6 via the first contact electrodes 10 and the measurement means 12. A calculation is made by the measurement means 12, and a control command signal 50 is sent to the neuromuscular stimulator means 46. The neuromuscular stimulator means 46 delivers a stimulation pulse or pulses 52 to the second contact electrodes 58.

Figure 15 shows a measurement wave form for use with a separate signal providing means 8 and a separate neuromuscular stimulator means 46, for example obtainable as shown in Figures 12 and 14. The neuromuscular stimulation pulses 52 are delivered with regular period. The measurement wave form 38 is applied between the stimulation pulses 52.

Figure 16 shows a realisation of a measurement wave form for using the component of the neuromuscular stimulation wave as may be employed using the apparatus shown in Figure 13. The measurement wave form is delivered in modulated bursts which are delivered with the neuromuscular stimulation pulse or pulses 52.

The apparatus of the present invention may be used for control of electrical stimulation of a muscle, for example a paralysed person's arm muscle, to ensure that the muscle extends but does not over-extend and perhaps damage itself. As indicated above, advantageously the same electrodes can be used for sensing and stimulation, as sensing can occur during the sub-second pauses, for example millisecond pauses, between each stimulation pulse.

The apparatus of the present invention may be used for monitoring muscle movement and/or use, for example for:

- (a) allowing remote health physicians to remotely check that a patient is performing appropriate exercises;
- (b) helping train athletes by monitoring muscle movement during exercise;
- (c) non-optical motion-capture systems, such as for controlling the movement of a virtual avatar in a virtual environment, so the avatar matches the movement of the computer user.

The apparatus of the present invention may be cheaper to manufacture than known apparatus with angle-meters or using optical data capture. For paralysis patients, it is much easier to calibrate apparatus of the present invention to prevent over-extension, compared to systems using angle-meters, gyroscopes etc, and the apparatus of the present invention is similarly cheaper. For sports and haptics applications, one benefit is that sensors can be integral and non-obstructing within a close fitting garment, so that again the apparatus of the present invention may be cheaper and simpler than with other known systems.

The muscle fibres may enable the measurement and react as stimulated because, at a molecular scale, the shape of elongated muscle fibres may give them a greater capacitive effect than non-elongated fibres.

The apparatus of the present invention may be used for therapeutic applications, for example involving electrical stimulation. Alternatively, the apparatus of the present invention may be used for non-therapeutic applications, for example measuring multiple muscle groups.

The garment may be made conductive with a conductive polymer or something similar. More than one muscle group may be monitored simultaneously. A single garment may have sensors for several muscle groups. The calibration step might be as simple as moving an arm or a joint to a position which fully extends the arm or other body part, and automatically logging the measured electrical changes to a maximum desirable predetermined value. A continuous re-calibration approach may be used if the measurement gets affected by small movements of the electrode position on an hourly basis or from day to day. Similarly, if each electrode is a close packed array of electrodes, a computer system may be employed to identify which electrode within each array has the most ideal position, based on measurements from that electrode having the greatest range of phase-lags, or some such similar method. Alternatively, in a stimulation embodiment, the apparatus of the present invention may detect which electrodes activate a muscle or joint most efficiently, and may then use these electrodes both for stimulation and sensing.

It is to be appreciated that the embodiments of the invention described above with reference to the accompanying drawings have been given by way of example only and that modifications may be effected. Thus, for example, the electrically conducting areas 18 may alternatively be separated by thinner

electrically conducting areas which are in a lower plane than the electrically conducting areas 18. The apparatus 2, 44, 54, 56 may be used with more than one muscle or muscle group. The apparatus 2, 44, 54, 56 is able to be used with the garment 14, or with different types of garments for different parts of the patient's body. The patient 6 may be any suitable patient including persons suffering muscle movement impairment, or athletes. The patient 6 may alternatively be an animal, for example a dog, cat or a race horse. Individual components shown in the drawings are not limited to use in their drawings and they may be used in other drawings and in all aspects of the invention.

CLAIMS

1. Apparatus for providing information on at least one muscle in a patient, which apparatus comprises:

- (i) signal providing means for providing measurement-enabling signals for the muscle;
- (ii) first contact electrodes for enabling the measurement-enabling signals from the signal providing means to be received by the patient;
- (iii) measurement means for measuring a parameter of the muscle, the parameter being such that it is affected by the measurement-enabling signals, and the parameter being such that it relates to at least one electrical property that is indicative of changes in tissue impedance caused by movement of the muscle; and
- (iv) a garment which is for being worn over the muscle in the patient and which comprises an array of separate electrically conducting areas,

and the apparatus being such that the first contact electrodes are able to be positioned on the garment at a predetermined precise position for obtaining the measured parameter and with the first contact electrodes

being in contact with those separate electrically conducting areas in the garment that are over the predetermined position.

2. Apparatus according to claim 1 in which the garment is made of a fabric which is stretchable or conformal.
3. Apparatus according to claim 1 or claim 2 in which the garment is a sleeve garment for being slid over a part of the patient.
4. Apparatus according to any one of the preceding claims in which the garment is a strap garment for being strapped around a part of a person.
5. Apparatus according to any one of the preceding claims in which the electrically conducting areas are spaced electrically conducting areas in the matrix.
6. Apparatus according to any one of the preceding claims in which the electrically conducting areas are woven into the garment or are moulded or printed into the garment.
7. Apparatus according to any one of the preceding claims in which the signal providing means is a separate signal generator.

8. Apparatus according to any one of claims 1 – 6 and including neuromuscular stimulator means for providing neuromuscular stimulation signals for the muscle.
9. Apparatus according to claim 8 in which the signal providing means and the neuromuscular stimulator means are provided as a single component.
10. Apparatus according to claim 8 in which the signal providing means is provided as a separate component from the neuromuscular stimulator means.
11. Apparatus according to any one of claims 8 – 10 in which the apparatus is used such that the measurement enabling signals for the muscle are imposed on the neuromuscular stimulation signals for the muscle.
12. Apparatus according to any one of claims 8 - 11 in which the first contact electrodes also enable the neuromuscular stimulation signals to be received by the patient.
13. Apparatus according to any one of claims 8 – 10 and including second contact electrodes which are separate from the first contact electrodes and which enable the neuromuscular stimulation signals to be received by the patient, the second contact electrodes being able to be positioned in the garment in a predetermined position for obtaining the neuromuscular stimulation and with the second contact electrodes being in contact with those

separate electrically conducting areas in the garment that area over the predetermined position.

14. Apparatus according to any one of the preceding claims in which the measurement-enabling signals have a wave form selected from at least one of:

- (a) a sine wave;
- (b) a square wave;
- (c) a triangular wave;
- (d) an arbitrary wave form shape;
- (e) repeated parts of similar or dissimilar wave forms;
- (f) a random wave form capable of being averaged; and
- (g) an impulse.

15. Apparatus according to claim 14 in which the random wave form is white noise.

16. Apparatus according to any one of the preceding claims in which the measurement means measures the parameter of the muscle by using an electrical property selected from at least one of:

- (a) phase shift;
- (b) amplitude;
- (c) slew rate;

- (d) a root mean squared value; and
- (e) impulse

17. Apparatus according to any one of the preceding claims and including sealing means for sealing electronically conducting parts on the garment, whereby the garment is able to be cleaned.

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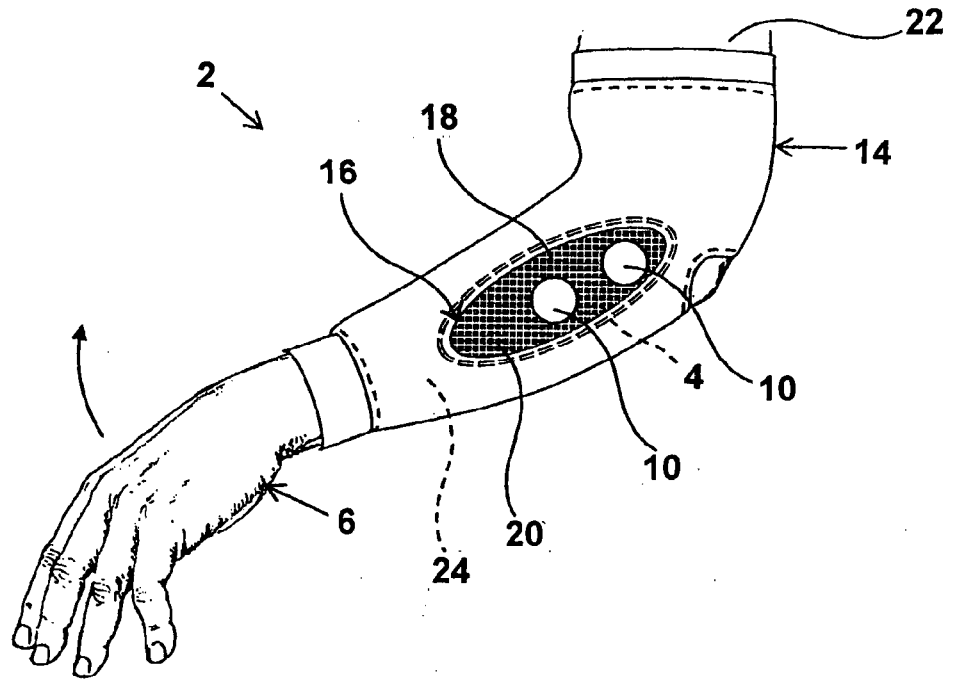


FIG. 1

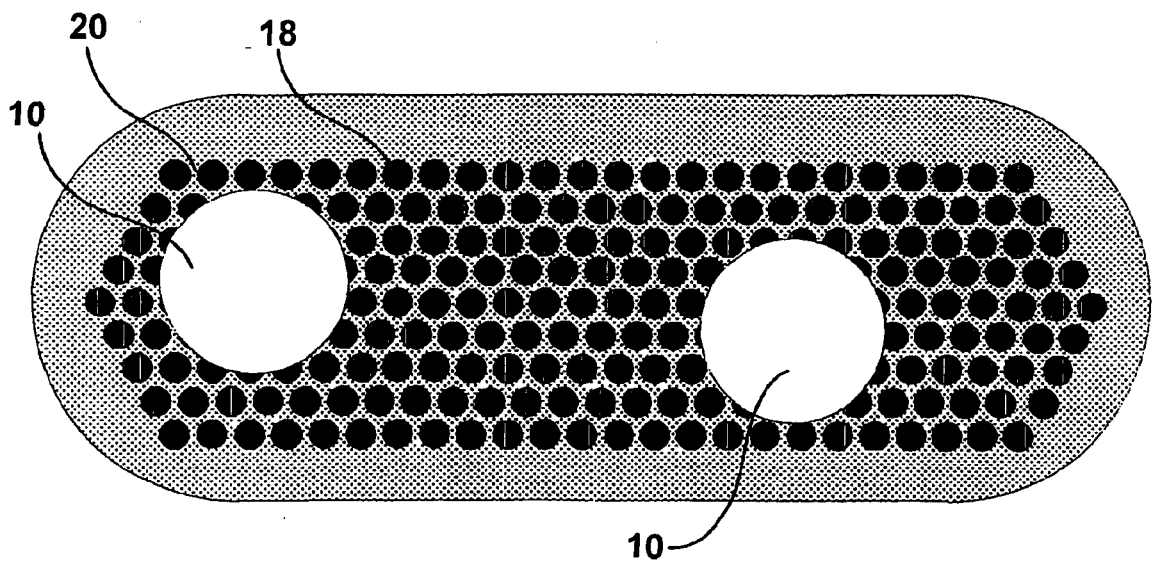


FIG. 2

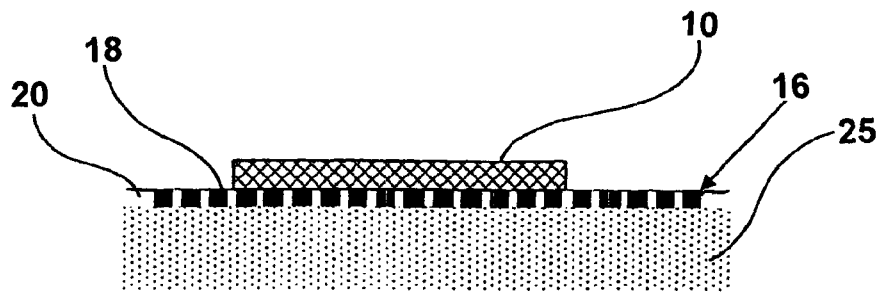


FIG. 3



FIG. 4

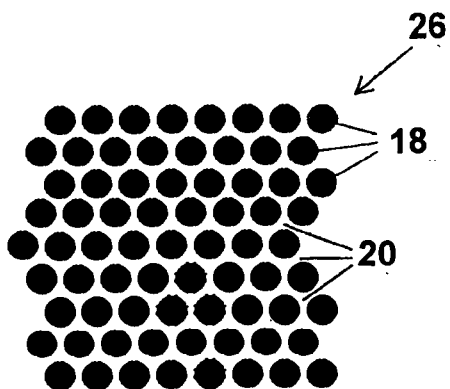


FIG. 5

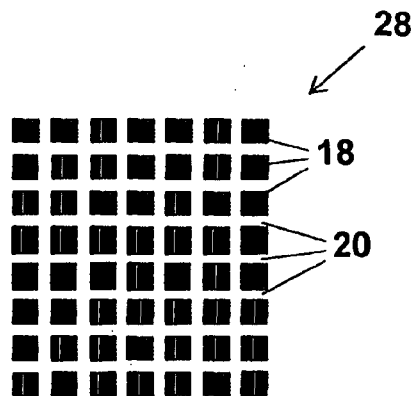


FIG. 6

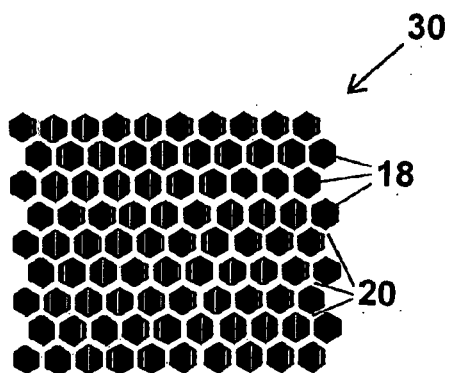


FIG. 7

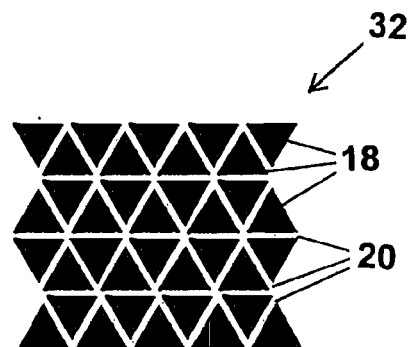


FIG. 8

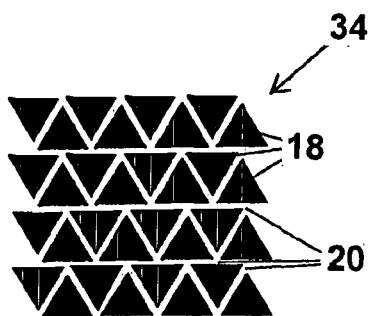


FIG. 9

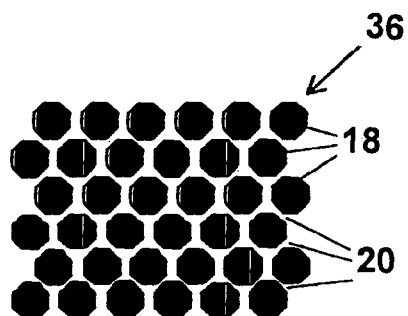


FIG. 10

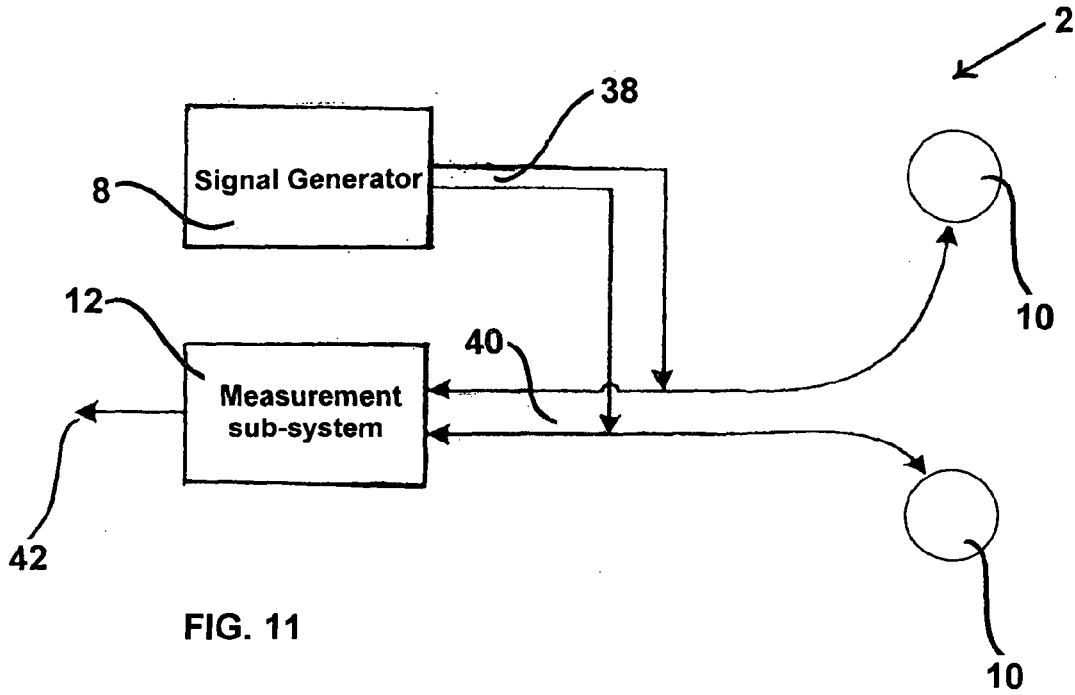


FIG. 11

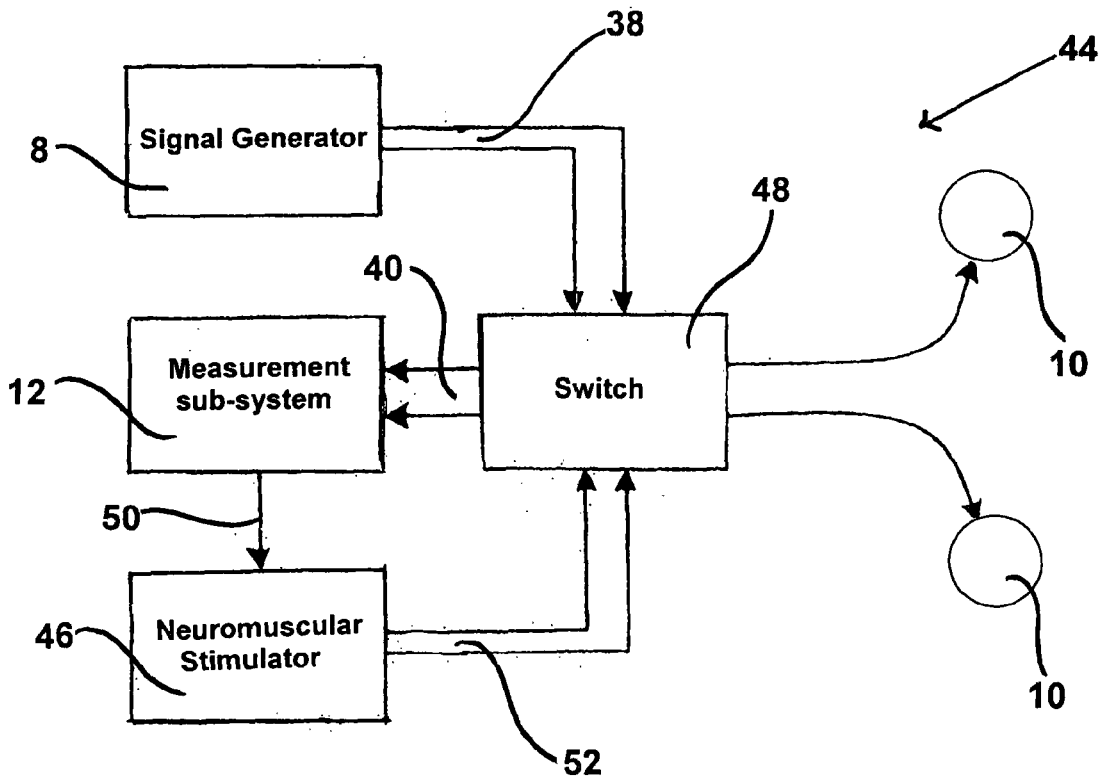


FIG. 12

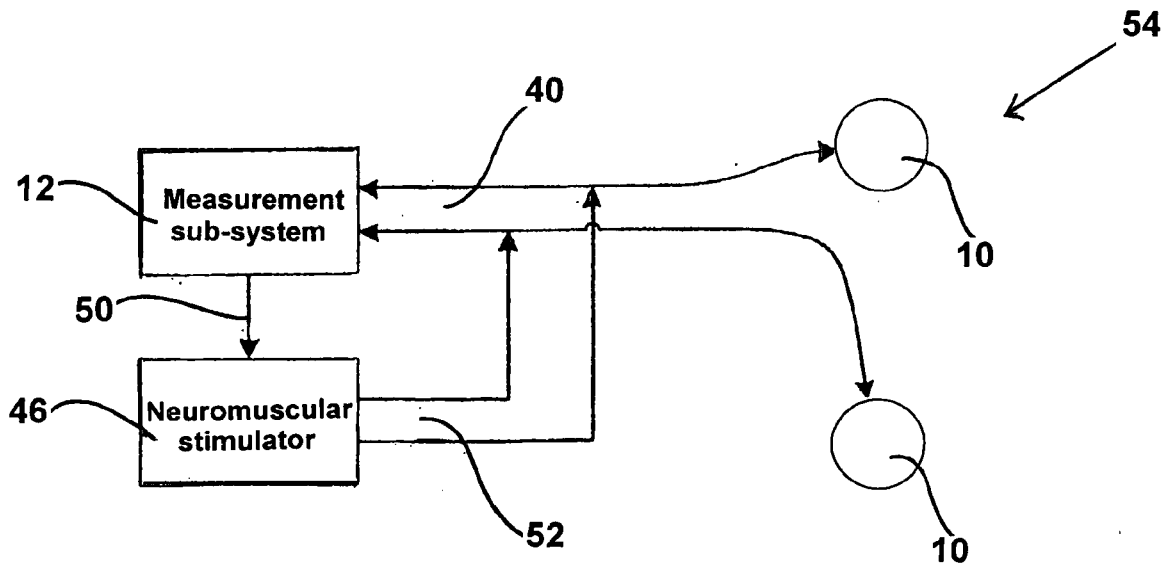


FIG. 13

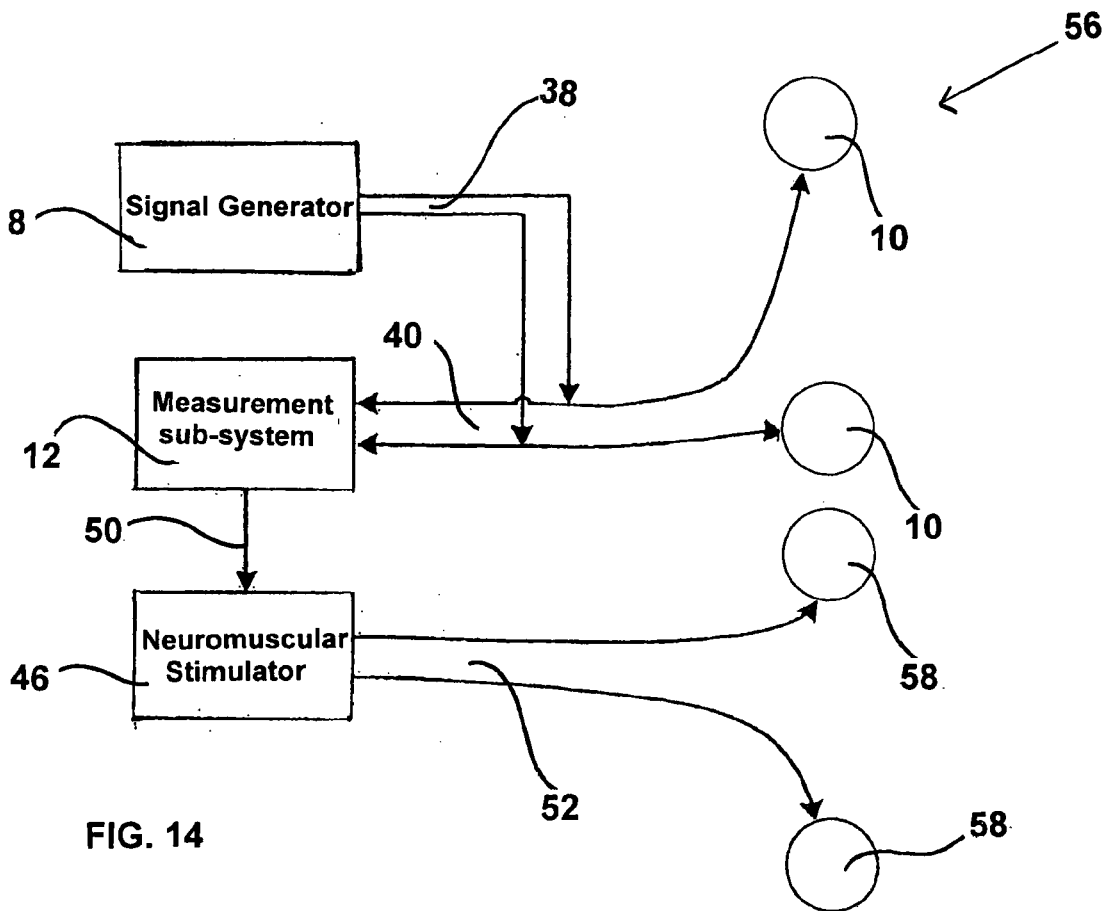


FIG. 14

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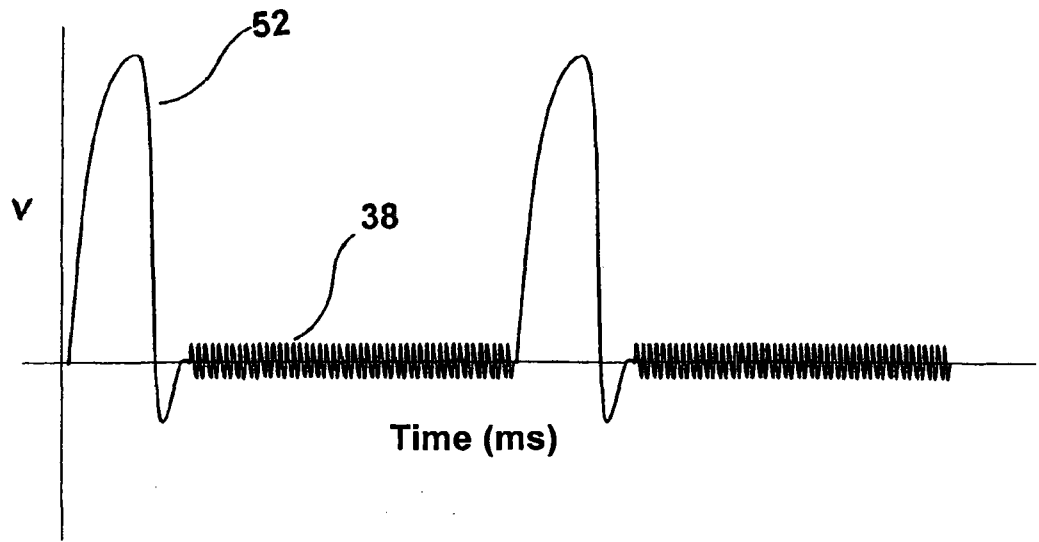


FIG. 15

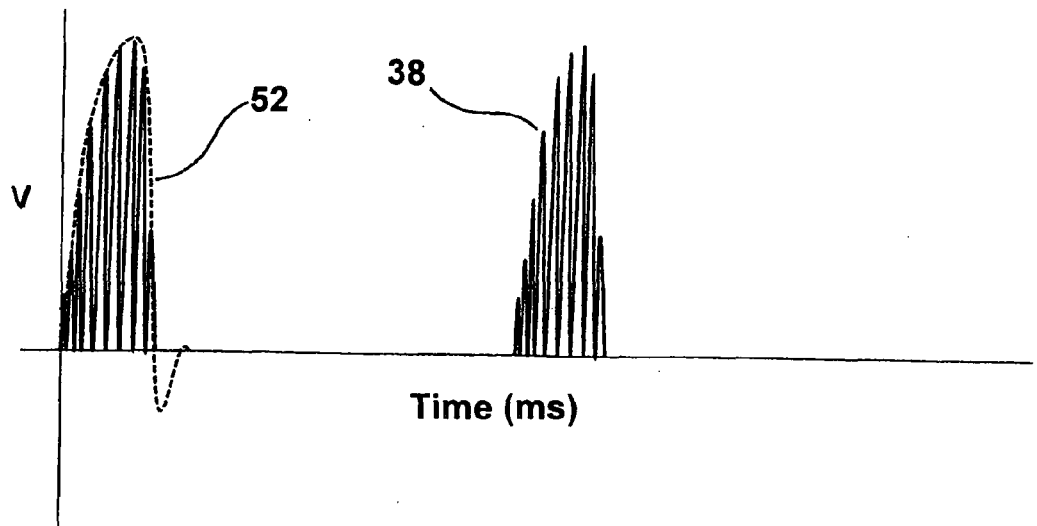


FIG. 16

INTERNATIONAL SEARCH REPORT

International application No
PCT/GB2013/000325

A. CLASSIFICATION OF SUBJECT MATTER
INV. A61B5/053 A61B5/00
ADD.

According to International Patent Classification (IPC) or to both national classification and IPC

B. FIELDS SEARCHED

Minimum documentation searched (classification system followed by classification symbols)
A61B

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

Electronic data base consulted during the international search (name of data base and, where practicable, search terms used)

EPO-Internal, WPI Data

C. DOCUMENTS CONSIDERED TO BE RELEVANT

Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X	WO 2008/075250 A1 (KONINKL PHILIPS ELECTRONICS NV [NL]; VAN HERK JOHANNES J [NL]; VAN LIE) 26 June 2008 (2008-06-26)	1-3,5-17
A	figures 2, 8 page 2, lines 3-5, 24-28 page 3, lines 16-18, 21-33 - page 4, lines 1, 2, 6-15 page 5, lines 26-31 page 6, lines 19-20 page 7, lines 14-20 page 8, lines 10-16 page 9, lines 24-33 page 10, lines 19-23 page 11, lines 29, 30 page 12, lines 6-8, 24-31 page 13, lines 6, 7 ----- -/--	4

Further documents are listed in the continuation of Box C.

See patent family annex.

* Special categories of cited documents :

- "A" document defining the general state of the art which is not considered to be of particular relevance
- "E" earlier application or patent but published on or after the international filing date
- "L" document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified)
- "O" document referring to an oral disclosure, use, exhibition or other means
- "P" document published prior to the international filing date but later than the priority date claimed

"T" later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention

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"&" document member of the same patent family

Date of the actual completion of the international search

28 August 2013

Date of mailing of the international search report

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Name and mailing address of the ISA/

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INTERNATIONAL SEARCH REPORT

Information on patent family members

International application No

PCT/GB2013/000325

Patent document cited in search report	Publication date	Patent family member(s)	Publication date
WO 2008075250 A1	26-06-2008	AT 489065 T	15-12-2010
		CN 101563056 A	21-10-2009
		EP 2097056 A1	09-09-2009
		JP 2010512827 A	30-04-2010
		US 2010087903 A1	08-04-2010
		WO 2008075250 A1	26-06-2008

专利名称(译)	用于提供关于患者中的至少一个肌肉的信息的装置		
公开(公告)号	EP2877088A1	公开(公告)日	2015-06-03
申请号	EP2013744768	申请日	2013-07-25
[标]申请(专利权)人(译)	南安普敦大学		
申请(专利权)人(译)	南安普顿大学学报		
当前申请(专利权)人(译)	南安普顿大学学报		
[标]发明人	CHAPPELL PAUL HAMMOND LANE RODNEY PAUL		
发明人	CHAPPELL, PAUL HAMMOND LANE, RODNEY PAUL		
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优先权	2012013592 2012-07-27 GB		
外部链接	Espacenet		

摘要(译)

用于提供关于患者(6)中的至少一个肌肉(4)的信息的装置(2),该装置(2)包括:(i)用于为肌肉(4)提供测量使能信号的信号提供装置(8);(ii)第一接触电极(10),用于使来自信号提供装置的测量使能信号能够被患者(6)接收;(iii)用于测量肌肉(4)的参数的测量装置(12),该参数使得其受到测量使能信号的影响,并且该参数使得其涉及至少一个电特性,即表示由肌肉运动引起的组织阻抗变化(4);(iv)衣服(14),其用于穿戴在患者(6)中的肌肉(4)上并且包括分开的导电区域(18)的阵列(16),并且装置(2)是这样,第一接触电极(10)能够在预定的精确位置定位在衣服(14)上,以获得测量的参数,并且第一接触电极(10)与第一接触电极(10)中的那些单独的导电区域接触。衣服(14)在预定位置上方。该装置任选地包括神经肌肉刺激器装置(46),用于为肌肉(4)提供神经肌肉刺激信号。