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(54) Title: METHOD AND SYSTEM FOR ALTERING BODY MASS COMPOSITION USING GALVANIC VESTIBULAR STIMULATION

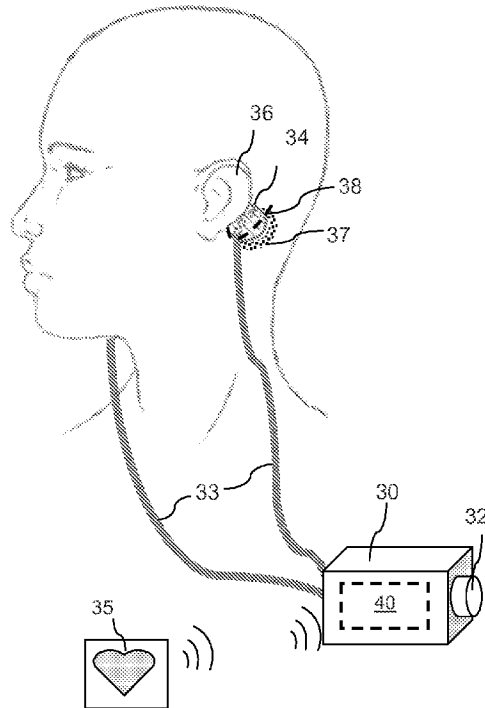


FIG. 5

(57) Abstract: A device and method are provided for altering body mass composition in a human subject by applying galvanic vestibular stimulation (GVS) using electrodes placed in electrical contact with the subject's scalp at a location corresponding to each of the subject's left and right vestibular systems. The current source include a feedback loop for measuring a resistance across the subject's scalp and adjusting a voltage output to maintain a constant current across the subject's scalp. GVS may be applied for a predetermined period of time at regular intervals.

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## METHOD AND SYSTEM FOR ALTERING BODY MASS COMPOSITION USING GALVANIC VESTIBULAR STIMULATION

### RELATED APPLICATIONS

5 This application claims the benefit of the priority of U.S. Provisional Application No. 61/771,766, filed March 1, 2013, which is incorporated herein by reference in its entirety.

### FIELD OF THE INVENTION

The present invention relates to a device and method for vestibular stimulation  
10 to produce physiological changes in an individual's body mass composition.

### BACKGROUND OF THE INVENTION

Obesity is a medical condition which involves the accumulation of excess body fat. It is defined by body mass index (BMI), which is a measure of body weight based upon an individual's weight and height. ( $BMI = \text{mass}(\text{kg})/(\text{height}(\text{m}))^2$ ).  
15 Obesity is defined, by both the World Health Organization and the National Institutes of Health, as a BMI greater than or equal to 30, and pre-obesity is defined as a BMI in the 25 to 30 range. Obesity is one of the leading preventable causes of death worldwide, and is thought to reduce life expectancy by around 7 years. Excess body fat in itself can also cause significant perceived issues with cosmesis in healthy  
20 individuals.

Many different techniques have been employed to assist individuals who are overweight to lose weight. These include multiple different types of diet, exercise regimes, weight loss medications and weight loss surgery. There is currently no easy or universally effective weight loss solution.

25 Osteoporosis is a disease of bones that is characterized by a reduction in bone mineral density (BMD), with the result that there is an increased risk of fracture. The World Health Organization defines osteoporosis as a BMD that is 2.5 standard deviations or more below the mean peak bone mass (average of young, healthy adults) as measured by dual energy X-Ray absorptiometry. The development of osteoporosis  
30 is determined by the interplay of three factors: first, an individual's peak BMD; second the rate of bone resorption; third, the rate of formation of new bone during remodelling. It is a particular health concern with aging populations in the developed

world, especially in post-menopausal women. A variety of pharmacological treatments have been employed to treat osteoporosis with the mainstay of current management being bisphosphonates, which alter the rate that bone is resorbed.

Centrifugation can in effect mimic a gravitational field greater than that  
5 experienced on the surface of the Earth (1G), referred to as “hypergravity” (Smith, 1992). It has been observed that chronic centrifugation of animals leads to an alteration of body mass composition (Fuller et al., 2000; Fuller et al., 2002). In particular, animals subjected to hypergravity via centrifugation exhibit a shift in “the proportional distribution of body mass between fat and fat-free components” (Fuller  
10 et al., 2000), with a reduction in body fat that is proportional to field strength (Fuller et al., 2002).

Hypergravity has been reported to specifically bring about a reduction in the body fat of chickens (Evans et al., 1969; Smith & Kelly, 1963; Smith & Kelly, 1965; Burton & Smith, 1996), hamsters (Briney & Wunder, 1962), other domestic fowl  
15 (Smith et al., 1975), rabbits (Katovich & Smith, 1978), mice (Oyama & Platt, 1967; Keil, 1969; Fuller et al., 2000; Fuller et al., 2002) and rats (Oyama & Platt, 1967; Oyama & Zeitman, 1967; Pitts et al., 1972; Roy et al., 1996; Warren et al., 1998). The observed decrease in body fat can be quite significant. For example, it has been reported that chickens will decrease from 30% body fat at 1G to 3% at 3G (Burton &  
20 Smith, 1996). Similarly, mice living at 2G showed approximately a 55% reduction in absolute and percentage carcass fat (Fuller et al., 2000). This seems to be accompanied by an increased usage of fatty acids as a metabolic substrate, and an increased metabolic rate (Fuller et al., 2006).

While marked loss of fat appears to be the principal change in body mass  
25 composition to hypergravity, and with it an increase in the relative size of the body’s fat-free component, specific changes to the muscles and bones of animals subjected to chronic centrifugation have also been noted by some authors. Small laboratory animals adapted to a 2G environment have been reported to increase their skeletal mass (as measured using body calcium content) by around 18% (Smith, 1992). Jaekel  
30 et al. (1977) also reported that prolonged centrifugation at 2.76G led to an increased bone mineral density in rat thigh bones.

The balance between flexor and extensor muscles has been observed to shift in response to hypergravity to favor muscles with an anti-gravity function (Smith, 1992). In domestic fowl on Earth the leg extensor:flexor muscle mass ratio is 0.85 but 2G altered this ratio to 1.17 (Burton & Smith, 1967; Smith, 1992). There also appears to be a functional difference in the muscles of animals exposed to hypergravity. Animals adapted to 2.5G have been reported to demonstrate a markedly increased exercise capacity (as measured by running to exhaustion), of about three-fold that of non-adapted controls, and an increased maximum oxygen uptake (Burton and Smith, 1967, 1996). Hamsters exposed to a 4G environment for 4 weeks were similarly found to have a greater resistance to fatigue in the gastrocnemius muscle and a 37% increase in the strength of its tetanic contraction (Canonica, 1966).

Functional adaptations in the muscles of rats adapted to hypergravity have been examined by analysis of the protein called myosin heavy chain (MHC) (Fuller et al., 2006). Adult rats exposed to 2G for eight weeks were found to have altered MHC characteristics in their soleus and plantaris muscles (Fuller, 2006). Soleus tends to have more slow-twitch fibers, which are better at endurance activities, and plantaris has relatively more fast-twitch fibers, which are better for sprinting but tend to fatigue more rapidly (Gollnick et al., 1974; Fuller et al., 2006). Fuller et al. (2006) found that the rats adapted to 2G had an increase in the slow twitch form of MHC (MHC1) in their soleus muscles, and a converse increase in the fast twitch form of MHC (MHC2b) in their plantaris muscles.

Several mechanisms have been proposed to explain these physiological changes, either alone or in conjunction, including: alterations in mitochondrial uncoupling proteins; fluid volume shifts; alterations in intracranial pressure; increased loading of skeletal muscles; altered feeding behavior; and activation of the vestibular system (Fuller et al., 2000; Fuller et al., 2002). The vestibular system, which is a major contributor to our sense of balance and spatial orientation, consists in each inner ear of three semicircular canals (which detect rotational movement) and the two otolith organs, termed the utricle and saccule, which detect linear acceleration and gravity (Khan & Chang, 2013). They are called otolith organs as they are fluid filled sacs containing numerous free moving calcium carbonate crystals – called otoliths –

which move under the influence of gravity or linear acceleration to act upon receptor cells to alter vestibular afferent nerve activity.

Experiments using mutant mice have suggested that the otolith organs are of particular importance in producing the physiological changes observed in animals subjected to chronic centrifugation. In the first experiment, wildtype mice and a type  
5 of mutant mice that lack otolith organs but have intact semicircular canals were subjected to 8 weeks of chronic centrifugation at 2G (Fuller et al., 2002). At the end of this period the percentage body fat was significantly reduced in the wildtype mice living at 2G compared to a control population living at 1G (8.5% cf 15.5%), and the  
10 percentage lean muscle mass was significantly increased compared to the control population (91.5% cf 83.1%). However, the mutant mice (lacking otolith organs) living at 2G showed no significant change in their body mass composition compared to mutant mice living at 1G.

The second study involved subjecting wildtype and mutant mice (without  
15 otolith organs) to just two hours of centrifugation at 2G (Fuller et al., 2004). In the wildtype mice, the authors reported widespread activation (as determined by c-fos upregulation) of a variety of brain structures known to be important in homeostasis and autonomic nervous system regulation including: the dorsomedial hypothalamus (a brain area thought to be of major importance in overseeing feeding behavior and in  
20 fixing a set point for body mass (Fuller et al., 2004)); the parabrachial nucleus; the bed nucleus of the stria terminalis; the amygdala; the dorsal raphe; and the locus ceruleus. These findings were not observed in the mutant mice.

The vestibular nuclei (which are located in the pons and medulla and receive input via the vestibular nerve from the vestibular system) are thought to project (both  
25 directly and indirectly via the parieto-insular vestibular cortex (PIVC)) to the brainstem homeostatic sites of the parabrachial nucleus (PB) and the peri-aqueductal gray (PAG) (see Chapter 1 and Chapter 3, Section 8 in doctoral thesis by McGeoch, 2010). The PB seems to act to maintain homeostasis – i.e., a stable internal physiological milieu – by integrating this vestibular input with sympathetic input (via  
30 lamina 1 spino- and trigemino-thalamic tract fibers) and parasympathetic input (via the nucleus of the solitary tract) (Balaban and Yates, 2004; Craig, 2007; Craig, 2009; McGeoch et al., 2008, 2009; McGeoch, 2010).

It is thought that the PB then acts to maintain homeostasis by means of behavioral, neuroendocrine, and autonomic nervous system efferent (i.e., both sympathetic and parasympathetic) responses (Balaban and Yates, 2004; McGeoch, 2010). Anatomically the PB projects to the insula and anterior cingulate, amygdala  
5 and hypothalamus. The insula and anterior cingulate are areas of cerebral cortex implicated in emotional affect and motivation, and hence behavior (Craig, 2009). The hypothalamus plays a vital role in coordinating the neuroendocrine system and, particularly via its dorsomedial aspect, oversees feeding behavior and fixes a set point for body mass composition (Balaban and Yates, 2004; Fuller et al., 2004; Craig,  
10 2007). The amygdala (together again with the hypothalamus and insula) is similarly known to be important in autonomic nervous system control. The PB also outputs to the PAG and basal forebrain, which are also involved in homeostasis (Balaban and Yates, 2004).

The vestibular system is also known to input to the rostral ventro-lateral  
15 medulla (RVLM), which is a major sympathetic control site, and it seems likely that any observed modulatory effect of vestibular stimulation on sympathetic function will, at least in part, be mediated via the RVLM (Bent et al., 2006; Grewal et al., 2009; James & Macefield 2010; James et al., 2010; Hammam et al., 2011). However, as the semicircular canals are not involved in modulating sympathetic outflow during  
20 vestibular stimulation (Ray et al., 1998), any sympathetic modulation arising from vestibular stimulation must be attributable to activation of the otolith organs (i.e., the utricle and saccule). It is known that white adipose tissue, which constitutes the vast majority of adipose tissue in the human body, is innervated by the sympathetic nervous system and that this innervation regulates the mass of the adipose tissue and  
25 the number of fat cells within it (Bowers et al., 2004).

The sympathetic nervous system is also known to innervate mature long bones and by this means plays a modulatory role in bone remodelling (Denise et al., 2006). Bilateral vestibular lesions in rats lead to a decrease in the mineral density of weight bearing bones (Denise et al., 2006). However, this reduction is prevented by the  
30 adrenoceptor antagonist propranolol (Denise et al., 2006), which suggests a direct interaction between the vestibular inputs and the sympathetic nervous system. Hence, it appears that the reported increase in bone mineral density in response to

hypergravity (Jaekel et al., 1977; Smith, 1992), may also be mediated by a vestibulo-sympathetic effect.

There are also data showing direct pathways connecting the vestibular nuclei with the dorsomedial hypothalamus (Cavdar et al., 2001), which is the part of the hypothalamus already mentioned as being specifically involved in regulating feeding behavior and setting a fixed point for body mass (Fuller et al., 2004).

The hormone leptin is secreted by fat cells and acts upon the hypothalamus to regulate food intake and energy expenditure. Leptin acts to suppress food intake and increase energy expenditure (Hwa et al., 1997), and as such plays a role in regulating body weight. Notably, vestibular stimulation has been found to cause an increase in leptin release (Sobhani, 2002; Sailesh & Mukkadan, 2014).

A chemical approach to vestibular stimulation may be based on betahistine, a partial histamine-3 (H3) receptor antagonist that has been used for some time to treat Meniere's disease. It is also known that by blocking presynaptic H3 receptors, betahistine causes an increased release of histamine and activation of H1 receptors, which is the opposite action to antihistaminic vestibular suppressants (Barak et al., 2008; Baloh & Kerber, 2011). Some early reports have suggested that, at least in certain subgroups, betahistine may be an effective weight loss medication (Barak et al., 2008). Conversely vestibular suppressant medications often lead to weight gain.

Various techniques have been used for research and clinical purposes to stimulate some or all of the components of the vestibular system in humans (Carter and Ray, 2007). These include: (1) Caloric vestibular stimulation, which involves irrigating the outer canal of the ear with warm or cold water or air and mainly stimulates the lateral semicircular canal of that ear; (2) Yaw head rotations, which activates both lateral semicircular canals; (3) Head-down rotation to activate otolith organs and also, initially, semicircular canals; (4) Linear acceleration, which activates otolith organs; (5) Off-vertical axis rotation (OVAR), which activates otolith organs; (6) Galvanic vestibular stimulation ("GVS"), which activates all five components of the vestibular apparatus simultaneously using an electrical current (Fitzpatrick & Day, 2004; St. George & Fitzpatrick, 2011); (7) Click induced vestibular stimulation using an auditory click (Watson & Colebatch, 1998); and (8) Neck muscle vibration induced vestibular stimulation (Karnath et al., 2002). Of these techniques, only one

offers the practical option of being produced commercially for home use without expert supervision -- GVS.

GVS involves stimulating the vestibular system through the transcutaneous application of a small electric current (usually between 0.1 to 3 milliamps (mA)) via two electrodes. The electrodes can be applied to a variety of locations around the head, but typically one is applied to the skin over each mastoid process, i.e., behind each ear. Some authors term this a “binaural application.” If a cathode and an anode are used with one placed over each mastoid, which is the most common iteration, then this is termed a bipolar binaural application of GVS. The current can be delivered in a variety of ways, including a constant state, in square waves, a sinusoidal (alternating current) pattern and as a pulse train (Petersen et al., 1994; Carter & Ray, 2007; Fitzpatrick & Day, 2004; St. George & Fitzpatrick, 2011).

An electronic appetite suppressant device known as the FOOD WATCHER™ was available on the market in the United Kingdom until recently. The premise behind the FOOD WATCHER™ was that it would act to electrically activate acupuncture points on the ears, with the consequence that a user’s appetite would be suppressed. Additionally it was argued that it may suppress appetite by activating the vagus nerve (Esposito et al., 2012).

The FOOD WATCHER™ electrodes were conically shaped plugs designed to be inserted into the external auditory canals (Esposito et al., 2012). The FOOD WATCHER™ is reported to have generated a “signal with amplitude of 40V, frequency of 50Hz and current of 40 mA through the ear plugs” (Esposito et al., 2012).

A study was carried out on 40 overweight and obese healthy volunteers to investigate the effectiveness of the FOOD WATCHER™ (Esposito et al., 2012). Ten volunteers received the FOOD WATCHER™ and a hypocaloric diet, ten received a hypocaloric diet alone, ten received the FOOD WATCHER™ and a high-protein diet, and ten a high protein diet alone. The authors found that “after 2 months of simultaneous treatment with electric stimulation and diet there was an average weight loss of 7.07 kg in the hypocaloric group and 9.48 kg in the high-protein group, whereas an average weight loss of 5.9 kg and 7.17 kg were observed with hypocaloric and high-protein diet alone, respectively”, leading the authors to conclude that

electrical stimulation through the ears may help with weight loss, particularly when used with a high-protein diet, possibly acting via a Yin-yang acupuncture energy balance.

Muscle sympathetic nerve activity (MSNA) to the blood vessels in skeletal  
5 muscle can be measured directly in man using microelectrodes. It has been reported that GVS delivered as square wave pulses (at 2 mA of 1 second duration) was ineffective at altering MSNA (Bolton et al., 2004; Carter & Ray, 2007). Conversely, delivering GVS (with an electrode over each mastoid) more dynamically is effective at modulating MSNA. This has been shown using both pulse trains (specifically 10,  
10 1ms pulses across 30ms and time-locked to the R wave of the electrocardiogram) (Voustianiouk et al., 2005), and sinusoidal GVS (-2 to 2 mA, 60-100 cycles, applied at administered bipolar binaural GVS ( $\pm$  2mA, 200 cycles) at frequencies of 0.2, 0.5, 0.8, 1.1, 1.4, 1.7 & 2.0 Hz, to 11 human volunteers while measuring their MSNA (Grewal et al., 2009).

15 Grewal et al. found a degree of cyclic modulation of MSNA at all frequencies, however, vestibular modulation of MSNA was significantly stronger at 0.2 Hz and significantly weaker at 0.8 Hz. This suggested “that low-frequency changes in vestibular input, such as those associated with postural changes, preferentially modulate MSNA.” Conversely, it was proposed that vestibular inputs around the  
20 frequency of the heart rate (i.e., 0.8 Hz, which is 48 beats per minute) compete with, and are inhibited by, the modulation of the MSNA by baroreceptors (pressure detecting mechanoreceptors in the walls of blood vessels), which are activated at the frequency of the heart rate.

The baroreceptor reflex is believed to act via the parasympathetic nervous  
25 system (including the vagus nerve and nucleus of the solitary tract) to inhibit the action of the RVLM. This inhibition may be mediated, at least in part, via the caudal ventrolateral medulla (Sved et al., 2000).

Additional evidence to support the argument that vestibular inputs with a  
30 frequency distinct from the cardiac frequency are more potent at modulating MSNA, is found in a study in which 8 human subjects were given sinusoidal GVS at their own cardiac frequency, and at  $\pm$ 0.1,  $\pm$ 0.2,  $\pm$ 0.3,  $\pm$ 0.6 Hz from this frequency (James &

Macefield, 2010). The authors report that the modulatory effect of the GVS on MSNA activity was impaired when its frequency was closer to the cardiac frequency.

The same authors also measured skin sympathetic nerve activity (SSNA), using microelectrodes, in 11 volunteers subjected to bipolar binaural GVS over the mastoid processes ( $\pm 2$  mA, 200 cycles) at 0.2, 0.5, 0.8, 1.1, 1.4, 1.7 and 2.0 Hz (James et al., 2010). Marked entrainment of GVS was found at all frequencies, although it was significantly weaker at 2.0 Hz. In contrast to the pattern observed with vestibular modulation of MSNA (Grewal et al., 2009), it was reported that the pulse related modulation of SSNA was greater at 0.8 Hz than at 0.2 Hz.

In a recent study, this group found that low frequency sinusoidal GVS (at 0.08, 0.13 and 0.18 Hz) caused two peaks of MSNA modulation (Hammam et al., 2011). This suggested that the primary peak occurs from the positive peak of the sinusoid in which the right vestibular nerve is hyperpolarized and the left depolarized, with the secondary peak of MSNA modulation occurring during the reverse scenario. This behavior was not observed at higher frequencies, possibly because there was insufficient time for a secondary peak to be produced. The authors suggest that this finding indicates “convergence of bilateral inputs from vestibular nuclei onto the output nuclei from which MSNA originates, the rostral ventro-lateral medulla.”

Various uses for vestibular stimulation have been described in related art, including: treating motion sickness (US Pat. No. 4,558,703 to Mark); headsets for stimulation in a virtual environment (US Pat. No. 6,077,237 to Campbell, et al.); counteracting postural sway (US Pat. No. 6,219,578 to Collins, et al.); to induce sleep, control respiratory function, open a patient’s airway and/or counteract vertigo (US Pat. No. 6,748,275 to Lattner, et al.); an in-ear caloric vestibular stimulation apparatus (US Pat. No. 8262717 to Rogers, et al.); and to alleviate anxiety (US Pat. No. 8,041,429 to Kirby).

Patent applications have been filed for the following: a method of delivering caloric vestibular stimulation (US Patent Publication 2011/0313498 to Rogers, et al.) and a system and method for reducing snoring and/or sleep apnea in a sleeping person, which may involve the use of GVS (US Patent Publication 2008/0308112 to Bensoussan). Chan, et al. have filed several patent applications for a variety of uses of GVS including: an adaptive system and method for altering the motion of a person

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(US Patent Publication 2010/0114256); a system for altering motional responses to sensory input (US Patent Publication 2010/0114255); a system and method for providing therapy by altering the motion of a person (US Patent Publication 2010/0114188); a system and method for providing feedback control in a vestibular stimulation system (US Patent Publication 2010/0114187); a system for altering the motional response to music (US Patent Publication 2010/011418); a system and method for game playing using vestibular stimulation (US Patent Publication 2010/0113150); a system and method of altering the motions of a user to meet an objective (US Patent Publication 2010/0112535); and a system and method of training to perform specified motions by providing motional feedback (US Patent Publication 2010/0112533).

GVS is also known to stimulate all components of the vestibular apparatus, including the two otolith organs, and dynamic forms of GVS (i.e., pulse train and sinusoidal) appear to be effective at modulating sympathetic activity. If bipolar binaural sinusoidal GVS is used, the modulation of MSNA is greater when it is administered at a frequency distinct from the cardiac frequency.

In spite of the many reported uses of GVS in the prior art, there has been no teaching or suggestion to apply GVS to alteration of body mass composition in humans. The present invention is directed to such an application.

## SUMMARY OF THE INVENTION

According to the present invention, a system and method are provided for galvanic vestibular stimulation to alter body mass composition in humans. In an exemplary embodiment, sinusoidal or pulse trains of galvanic current are applied via electrodes applied to a subject's scalp to stimulate the otolith organs and activate the vestibular system. The alteration of body mass composition may include one or more of the following effects: a decrease in body fat; a relative increase in lean muscle mass; and an increase in bone mineral density. The present invention may be used to treat obesity, diseases associated with obesity (e.g., type 2 diabetes mellitus and hypertension), osteoporosis, or it may be used as an aid in physical training to improve relative lean muscle mass and improve the exercise capacity of that muscle.

In an exemplary embodiment, vestibular stimulation, preferably via GVS (likely administered in a sinusoidal or pulse-train manner), is applied to modulate

body mass composition in order to bring about: a decrease in total body fat; an increase in lean muscle mass; and an increase in bone mineral density. This effect will likely take place via activation of the otolith organs of the inner ear by GVS and subsequent modulation of sympathetic nervous system activity, which is likely to be mediated via the RVLM. Additionally, this effect may also involve brain structures such as brainstem homeostatic sites (specifically the PB, PAG), the PIVC, amygdala, insula and the hypothalamus. The effect may also be mediated via an effect on the release of certain hormones, such as leptin. The efficacy of the invention is likely to be greater if bipolar binaural GVS (with an electrode over each mastoid process) is administered in a dynamic manner (e.g. sinusoidal or pulse train).

In one aspect of the invention, a device for altering body mass composition in a human subject includes electrodes disposed in electrical contact with the subject's scalp at a location corresponding to each of the subject's left and right vestibular system; and a current source in electrical communication with the electrodes for applying galvanic vestibular stimulation (GVS) to the subject. In one embodiment, the current source produces a constant current within a predetermined voltage range. The current source may produce a current having alternating polarity. The current source may further include a feedback loop for measuring a resistance across the subject's scalp and adjusting a voltage output to maintain a constant current across the subject's scalp. The current produced by current source may be within a range of 0.001 mA to 5 mA. The current produced by the current source may be sinusoidal with a frequency that is less than the subject's cardiac frequency.

In another aspect of the invention, a method for altering body mass composition in a human subject comprises applying galvanic vestibular stimulation (GVS) to the subject. The GVS can be applied by disposing an electrode on the subject's scalp proximate to each mastoid process. The GVS may be a current having a constant level and an alternating polarity. In one embodiment, the constant current level can be maintained by a feedback loop adapted to measure a resistance across the subject's scalp and adjust a voltage output to maintain the current level. The GVS may be a sinusoidal current having a frequency that is less than the subject's cardiac frequency. The GVS may be applied for a predetermined period of time at a regular interval, which may be daily, weekly, or a combination thereof.

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In yet another aspect of the invention, a method of decreasing total body fat in a human subject in need thereof comprises applying galvanic vestibular stimulation (GVS) to the subject. Still another aspect of the invention is a method of increasing relative percentage lean muscle mass in a human subject in need thereof by applying galvanic vestibular stimulation (GVS) to the subject. In a further aspect of the invention, a method of increasing bone mineral density in a human subject in need thereof includes applying galvanic vestibular stimulation (GVS) to the subject.

#### BRIEF DESCRIPTION OF THE DRAWINGS

The present invention will be better understood from the following detailed description of some preferred embodiments of the invention, taken in conjunction with the accompanying drawings, in which like numbers correspond to like parts, and in which:

FIG. 1 is a schematic diagram of an exemplary stimulator circuit.

FIG. 2 is a schematic diagram of an alternative embodiment of the stimulator circuit with a gain control component.

FIG. 3 is a schematic diagram of a second alternative embodiment of the stimulator device.

FIGs. 4A and 4B illustrate exemplary wave forms generated by the device.

FIG. 5 is a diagram showing an exemplary GVS electrode placement.

FIG. 6 is a diagram illustrating the vestibular system of the left inner ear.

FIG. 7 is a sample report showing the results of a first DXA scan of a human subject.

FIG. 8 is a sample report showing the results of a second DXA scan of the same human subject following a series of GVS stimulations.

#### DETAILED DESCRIPTION

FIGs. 1 and 2 illustrate one possible embodiment of the GVS circuitry that can be employed to carry out the method of the present invention. The device includes a source of time-varying galvanic current that may be software programmable using a microcontroller.

FIG. 1 illustrates the basic components of an embodiment of the stimulation device 20, which includes an operational-amplifier (“op-amp”) based constant-current

source. A voltage is placed across the scalp 10 through electrodes 4 and 6 and measured by the op-amp 12. In the exemplary embodiment, op-amp 12 may be a general purpose operational amplifier, an example of which is the LM741 series op-amp, which is widely commercially available. Selection of an appropriate operational amplifier will be within the level of skill in the art. If the voltage returning from the scalp 10 to pin 2 (inverting input) of op-amp 12 is different than the reference voltage +9V at pin 3 (non-inverting input), the operational amplifier draws from the +18V input through pin 7 to increase the amount of voltage output at pin 6, thereby increasing the current across the scalp 10 to maintain a constant current level. Load resistor 16 is 250 ohms. Adjustment of potentiometer 14 provides gain control by decreasing the voltage input into op-amp 12 at pin 2, thus controlling the amount of current flowing across the scalp. In the preferred embodiment, the +9V and +18V inputs are provided by one or more batteries (not shown), or a conventional DC converter may be used with appropriate safety provisions.

The schematic in FIG. 2 adds control components to the basic stimulator circuit 20 of FIG. 1. Transistor 22, powered by the pulse-width-modulation (PWM) output (MOSI (master output/slave input, pin 5) of an ATtiny13 microcontroller 24 (Atmel Corporation, San Jose, CA) or similar device, may be used to control the gain of the stimulator. The PWM causes the transistor to draw more or less of the voltage entering the Op-Amp 12 (pin 2) to ground, thus modulating the amount of current flowing across the scalp.

In a preferred embodiment, the device components and any external interfaces will be enclosed within a housing 30 (shown in FIG. 5) with appropriate user controls 32 for selecting stimulation parameters as appropriate. Note that a knob is shown for illustrative purposes only and that other types of controls, including switches, buttons, pressure bumps, slides, touch screens or other interface devices may be used. Optional design components that may be added to expand the functionality of the device include a memory storage device, such as a memory card or electrically erasable programmable read-only memory (EEPROM), which will allow the time, duration, and intensity of stimulations to be recorded. This can be accomplished by programming the microcontroller 24 to output a logic-level 3.4V pulse (TTL (transistor-transistor logic)) from the remaining digital out (MISO (master input/slave

output, pin 6) to a secure digital (SD) memory card, EEPROM, USB flash drive or other data storage device via an appropriate port on the device housing. Additionally, the +18V input may be derived by integrating a charge pump, or DC-DC step-up converter, such as the MAX629 or MAX1683 (not shown). This design feature would  
5 have the benefit of reducing the size of the device by producing the necessary +18V input from smaller batteries, which can be disposable or lithium ion rechargeable. Additional features may include wireless communication circuitry, as is known in the art, for programming and/or data collection from a remote computing device, which may include a personal computer, smart phone or tablet computer.

10 Other functions for implementing GVS in the present invention may include the ability to pulse the current at precise intervals and durations, in a sinusoidal wave with adjustable amplitude and period, and even switch polarity at precise intervals.

Additional options for facilitating and/or enhancing the administration of GVS may include a built-in biofeedback capability to adjust the stimulation parameters for  
15 optimal effect based on signals generated by sensors that monitor the subject's activity and/or biometric characteristics, such as motion, position, heart rate, etc. For example, real-time heart measured by a heart-rate sensor or monitor can be used as input into the GVS device, triggering an automatic adjustment of the sinusoidal GVS frequency to an appropriate, possibly pre-programmed, fraction of the cardiac  
20 frequency. Real-time data on the user's motion or position measured by accelerometers may also be used as input to control stimulation, to improve effectiveness and safety. For example, treatment could be terminated if excessive motion or change in the user's position is detected, or the user can be alerted about changes in position that could have adverse effects. The heart rate sensor/monitor  
25 and/or accelerometers may be separate devices that communicate with the inventive GVS device through a wired or wireless connection. Alternatively, sensors may be incorporated directly into the GVS device to form a wearable "sense-and-treat" system. As new sensors are developed and adapted to mobile computing technologies for form "smart", wearable mobile health devices, a "sense-and-treat" GVS device  
30 may provide closely tailored stimulation based on a wide array of sensor data input into the device.

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FIG. 3 schematically illustrates an exemplary prototype of the inventive device 40 implemented using the widely commercially-available ARDUINO<sup>®</sup> Uno single board microcontroller 42 (Arduino, LLC, Cambridge, MA), which is based on the ATmega328 microcontroller (ATMEL<sup>®</sup> Corporation, San Jose, CA).  
5 Microcontroller 42 includes fourteen digital input/output pins (of which six can be used as pulse width modulation (PWM) outputs), six analog inputs, a 16 MHz ceramic resonator, a USB connection, a power jack, an ICSP header, and a reset button. The +14.8 V DC power to the circuit is provided by batteries 49. For example, four lithium ion batteries, each providing 3.7V (1300mAh) are used, and are  
10 preferably rechargeable via charging port 51.

The PWM allows the output waveform to be accurately controlled. In this case, the waveform takes a repeating half-sine wave pattern in a positive deflection, as shown in FIG. 4A. The frequency has been predefined as 0.5Hz, but may be set to a different value by manual control or in response to input from a sensor, such as a  
15 heart rate sensor (see, e.g., FIG. 5). The user can manually control the amplitude by adjusting the potentiometer 48, allowing a range of 0 to 14.8V to be supplied to the electrodes. This adjustment may be effected by rotating a knob, moving a slide (physically or via a touch screen), or any other known user control mechanism. Alternatively, the potentiometer setting can automatically adjust in response to an  
20 input signal from a sensor. Relay 44 communicates the voltage adjustment to a graphical display 45 to provide a read-out of the selected voltage and/or current.

A relay 46 may be employed to effectively reverse the polarity of the current with every second pulse. The effect of this is shown in FIG. 4B, where the sinusoidal pattern changes polarity, thus generating a complete sine waveform to produce  
25 alternating periods of stimulation, on the order of 1 second in duration, to the left and right mastoid electrodes 50L and 50R.

The device may optionally include a three color LED 52 that provides a visual display of device conditions, i.e., diagnostic guidance, such as an indication that the device is working correctly or that the battery requires recharging.

30 Optional design components may include a touch screen configuration that incorporates the potentiometer controls, a digital display of voltage and current, plus other operational parameters and/or usage history. For example, remaining battery

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charge, previous stimulation statistics and variations in resistance could be displayed. Additional features may include controls for alterations in the waveform such as change of frequency and change of wave type (for example square, pulse or random noise). The ARDUINO<sup>®</sup> microprocessor platform (or any similar platform) is ideally  
5 suited to incorporate feedback control or manual control of frequency, intensity or other stimulation parameters based on an external signal source. For example, the ARDUINO<sup>®</sup> microprocessor platform, if provided with BLUETOOTH<sup>®</sup> capability, can be wirelessly controlled by an IPHONE<sup>®</sup>, ANDROID<sup>®</sup>, or other smart phone, laptop or personal computer, tablet or mobile device, so that the touchscreen of the  
10 mobile device can be used to control and/or display the GVS stimulation parameters rather than requiring a dedicated screen on the device. The mobile device may also be configured to store and analyze data from previous stimulations, providing trends and statistics about long periods of stimulation, such as over 6 months. Applications of this could allow for programs to monitor and guide users on their progress and goals,  
15 highlighting body measurements and changes in weight relative to the periods of stimulation.

An exemplary operational sequence for the embodiment of FIG. 3 for use in effecting an alteration in body mass composition may include the following steps:

1. When the push button power switch 41 is activated, the battery(ies) 49  
20 supply 5 volts DC to the microprocessor 42 through a 5 volt regulator and a 1 amp fuse (shown in the figure but not separately labeled.)
2. The LED 52 will flash green three times to indicate the power is "on". If the blue light flashes the battery needs charging. While the voltage is supplied to the electrodes 50L and 50R, the LED 52 will flash red at  
25 regular intervals, e.g., 30 seconds to a minute.
3. The microprocessor 42 generates a 0.75 VDC half wave sign wave. The voltage is amplified to 14.8 volts by the amplifier. The sine wave completes one-half cycle in 1 second (i.e., the frequency of the sine wave is 0.5Hz). The voltage can be varied by the potentiometer 48 from 0 to  
30 14.8 volts.
4. After a half cycle is completed, relay 46 switches polarity of the electrodes 50L, 50R and the microprocessor 42 sends another half cycle. The relay 46

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again switches polarity and continues for as long as the unit is “on”. This sends a full sine wave of up to  $\pm 14.8$  VDC to the electrodes, with the full voltage swing modulated by the potentiometer 48.

- 5           5. A digital display 45 provides a visual indication of the voltage and current delivered to the electrodes 50L, 50R. Depending on the size and complexity of the display, voltage and current values may be displayed simultaneously or alternately for a short duration, e.g., 3 seconds.

Other device options may include user controls to allow the current to be pulsed at precise intervals and durations, a sinusoidal wave to be generated with  
10 adjustable amplitude and period, and/or to switch polarity at precise intervals. External control and monitoring via a smart phone or other mobile device as described above may also be included. Further input and processing capability for interfacing and feedback control through external or internal sensors may be included.

FIG. 5 illustrates an exemplary GVS electrode 34 positioned on the skin  
15 behind the pinna of the left ear 36, and over the left mastoid process, of a subject to be treated. The mastoid process is represented by dashed line 38. The right electrode (not shown) would be placed in the same manner on the skin over the right mastoid process and behind the right pinna. It should be noted that the illustrated placement of the electrodes is provided as an example only. In fact, laterality of the electrode  
20 application, e.g., electrodes precisely over both mastoid processes, is not believed to be critical, as long as each electrode is in sufficient proximity to the vestibular system to apply the desired stimulation. The electrodes 34 are connected to stimulation device 40 (inside housing 30) by leads 33. Manual control means, illustrated here as a simple knob 32, may be operated to control the current or other parameters. As  
25 described above, alternative control means include a slide, touch screen, buttons or other conventional control devices. External control signals, for example, a signal from a heart rate monitor 35, may be input into the device either wirelessly, as illustrated, or by leads running between the sensor and the device. Electrodes such as the widely commercially available 2×2 inch platinum electrodes used for  
30 transcutaneous electrical nerve stimulation (TENS) may be used in order to minimize any possible skin irritation. A conducting gel 37 may be applied between the

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subject's scalp and the contact surface of the electrodes to enhance conduction and reduce the risk of skin irritation.

The amount of current the subject actually receives depends on the scalp resistance ( $I_{\text{scalp}} = V_{\text{electrodes}}/R_{\text{scalp}}$ ), which may vary as the user perspires, if the electrode position changes, or if contact with the skin is partially lost. It appears that the current levels quoted in the literature could only be delivered if the scalp resistance was much lower than it actually is. Measurements conducted in conjunction with the development of the inventive method and device indicate that the trans-mastoid resistance is typically between 200 to 500 k-Ohm. Thus, if a GVS device were actually being used to deliver 1 mA, the voltage would be between 200 to 500V according to Ohm's law. The battery-powered devices that are usually used to administer GVS are simply not capable of generating such an output. Hence, the existing reports appear to be inaccurate with regard to the actual current being delivered in GVS.

Prior art designs lack consideration for each subject's unique scalp resistance, and therefore may not deliver an effective current to each patient. In the present invention, this limitation can be overcome by taking into account inter-subject scalp resistance variability as well as compensating for fluctuations in the scalp resistance that may occur throughout the procedure. To compensate for slight and fluctuating changes in scalp resistance during the administration of current, the inventive GVS device may include an internal feedback loop that continuously compares the desired current against the actual measured current across the scalp and automatically compensates for any differences. If  $R_{\text{scalp}}$  increases, the  $V_{\text{electrodes}}$  increases to compensate. Conversely, voltage decreases when  $R_{\text{scalp}}$  drops. This dynamic feedback compensation loop provides constant current across the scalp for the duration of the procedure regardless of fluctuating changes in electrode-scalp impedance.

FIG. 6 illustrates the vestibular system of the left inner ear. The cochlea 68, which is the peripheral organ of hearing, is also shown. It demonstrates: the anterior 62, posterior 67, and horizontal 63 semicircular canals, which transduce rotational movements; and the otolith organs (the utricle 66 and saccule 65), which transduce linear acceleration and gravity. Without intending to be bound by any theory, it is believed that the otolith organs mediate any change in body mass composition that

GVS evokes. The vestibulocochlear nerve 64 (also known as the eighth cranial nerve) is composed of the cochlear nerve (which carries signals from the cochlea), and the vestibular nerve (which carries signals from the vestibular system).

#### Validation

5 Performance of the present invention was evaluated using dual energy x-ray absorptiometry (DXA), a technique that was originally developed to determine bone mineral density (BMD) and to aid in the management of osteoporosis. More recently, the technique has been expanded to include the analysis of fat mass and lean body mass in addition to BMD. The DXA machine emits alternating high and low energy  
10 x-rays that produce precise, high quality images. The use of a fan beam allows decreased scan times so that scans can be completed within seconds or minutes.

The basic principle of DXA data acquisition is based on the differences between bone and soft tissue attenuation at the high and low x-ray levels. As the x-ray beam passes through the subject, detectors register the varying levels of x-rays that  
15 are absorbed by the anatomical structures of the subject. The raw scan data, which includes values of tissue and bone, are captured and sent to a computer. An algorithm interprets each pixel, and creates an image and quantitative measurement of the bone and body tissues.

Whole body DXA scans using a HOLOGIC<sup>®</sup> Discovery W<sup>™</sup> DXA scanner  
20 were conducted to determine bone mineral density, lean mass and whole body fat. The technique has a precision error (1SD) of 3% for whole body fat and 1.5% for lean mass. The *in vivo* precision for the measurement of bone density using the DXA technique is 0.5 – 1.5% at the lumbar spine and the standard deviation of the lumbar spine bone density is 0.01 g/cm<sup>2</sup>. The radiation risk associated with the proposed  
25 protocol used is small and in cumulative total is equal to 0.26 mSv for each subject. This amount of radiation exposure is low, typically less than what one would receive from one year of natural exposure, i.e., around 1.6 mSv.

A comparable commercially available GVS device sold under the trademark VESTIBULATOR<sup>™</sup> (Good Vibrations Engineering Ltd. of Ontario, Canada) has  
30 previously been used in a number of research studies at other institutions. (Barnett-Cowan & Harris, 2009; Trainor et al., 2009.) This device functions with 8 AA batteries, so that the voltage can never exceed 12 V. According to the manufacturer's

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specifications, the maximum current that this device can deliver is 2.5 mA. The present invention uses a more user-friendly device (e.g., the delivered current can be adjusted using a controller (knob, slide, or similar) on the side of the housing, in comparison to the VESTIBULATOR™, where a similar adjustment can only be carried out by first writing a MATLAB® script and then uploading it remotely, via  
5 BLUETOOTH®, in order to reprogram the VESTIBULATOR's™ settings.)

Due to the very small currents used during GVS, the technique is believed to be safe (Fitzpatrick & Day, 2004; Hanson, 2009). In particular, although electrical current can lead to cardiac arrhythmias, including ventricular fibrillation, the  
10 threshold for such an occurrence is in the 75 to 400 mA range, well above the current levels the battery powered GVS devices can deliver. Furthermore, the electrodes will only be applied to the scalp, such as shown in FIG. 5, and nowhere near the skin over the chest.

Resistive heating can occur with high voltage electrical stimulation of the skin.  
15 However, the voltage and current (usually below 1mA) delivered during GVS are well below the levels that pose this risk. Nonetheless, skin irritation can occur due to changes in pH. This may be mitigated by using large surface area (approximately 2 inch diameter) platinum electrodes and aloe vera conducting gels.

It may be desirable to monitor the subject's heart rate (HR) to determine the  
20 cardiac frequency during GVS treatment. The cardiac frequency can then be used to alter the frequency of the sinusoidal GVS so as to maintain a certain ratio between the cardiac frequency and the frequency of the sinusoidal GVS to avoid interference with baroreceptor activity. For example, a sinusoidal GVS frequency to cardiac frequency ratio of 0.5 would be appropriate.

25 During administration of GVS, one platinum electrode is attached to the skin over one mastoid and the other electrode attached to the skin over the other, as shown in FIG. 5. The electrodes may be coated with conducting gel containing aloe vera. The device is activated to deliver a current of approximately 0.1 mA (given a trans-mastoid resistance of about 500 kOhm) with a sinusoidal waveform at 0.5Hz. A  
30 typical current range for the device would be around 0.001 mA to 5 mA. The subject should remain seated or lying flat throughout the session to avoid mishap due to altered balance during vestibular stimulation. The device is set up to automatically

stop after one hour however, the subject may discontinue the treatment sooner if desired. The subject should remain seated until their balance has returned to normal, which should occur within a short period of time after the GVS device has been turned off.

5 Example 1 – 23 Year Old Female Subject

Data accrued for one human subject support the use of GVS as an effective approach for altering body mass composition to reduce total body fat and increase lean muscle mass. The subject was a Hispanic female born in 1989 and at the time of the study was 23 years old. A cumulative total of 20 hours of GVS was administered  
10 between 8 October 2012 and 7 December 2012. Over this two month period, the subject received one hour of GVS on each stimulation day. No GVS session exceeded one hour on any stimulation day.

At the start and completion of the study (after providing a negative pregnancy test), the subject underwent DXA scans as described above. The first DXA scan was  
15 carried out on the day of the first GVS session (before the session) and the second scan was carried out five days after the final GVS session. In order to ensure a constant hydration status, the subject was instructed not to exercise within 12 hours of the DXA scans and to refrain from consumption of alcohol, nicotine, and caffeinated beverages. The subject reported that she was at the same stage of her menstrual cycle  
20 at the time of each scan. The subject was blinded as to whether she was receiving an experimental or placebo procedure.

The GVS was administered using the bipolar binaural method with an electrode placed on the skin over each mastoid process (see FIG. 5). A linear stimulus isolator from World Precision Instruments (A395D) was used to administer the  
25 stimulus, and a 0.5Hz sinusoidal waveform was imposed on this stimulus by a signal generator from BK Precision (Model 4010A). The subject was seated with her eyes open throughout the administration. The subject's approximate trans-mastoid resistance (after preparing the skin with micro-abrasive gel) was approximately 500 kOhm. To achieve the desired level of stimulation, the current delivered throughout  
30 each of the GVS sessions was approximately 0.1mA. The subject reported being aware of a swaying sensation during each stimulation session. The subject made no

changes to her dietary habits and did not engage in exercise during the study period. She was on no regular medications.

The report for the initial baseline DXA scan is provided in FIG. 7. Prior to treatment, testing indicated that the subject had a total body fat of 32947.4 g; a total  
5 combined bone mineral content (BMC) and lean muscle mass of 49799.3 g; and a percentage body fat of 39.8%. The second DXA scan performed after conclusion of the treatment period produced the results shown in FIG. 8. The post-treatment results indicated total body fat of 31839.9g; a total combined BMC and lean muscle mass of  
10 51890.4g; and a percentage body fat of 38.0%. (The BMC is directly proportional to the BMD, which as described above is used in the diagnosis of osteoporosis).

Between the two scans, the subject's combined BMC and lean muscle mass increased by 2091.1g and total body fat decreased by 1107.5g. Compared to the baseline scan, this represents an increase in combined BMC and lean muscle mass of  
15 4.2% and a decrease in total body fat of 3.4%. The subject's ratio of total fat to combined BMC and total lean muscle mass improved from 0.66 to 0.61. The data from this subject are thus supportive of the method of using GVS to alter body mass composition as described.

The inventive system and method are based on a novel use of vestibular stimulation, in particular, galvanic vestibular stimulation, to produce physiological  
20 changes in an individual human's body mass composition. The application of GVS as described herein simulates some of the effects of hypergravity, providing a safe, simple, drug-free approach to reduce body fat, increase lean muscle mass and increase bone density. The simplicity of the device and its operation makes it possible for any individual wishing to modify his or her body mass composition, regardless of whether  
25 for health, aesthetic, or athletic performance reasons, to administer stimulation in the privacy of their home. The device may also be used in a medical facility such as a doctor's office, clinic, or physical therapy facility to treat obesity and associated diseases, treat or prevent osteoporosis, and assist in physical training or recovery from injury.

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CLAIMS

1. A device for altering body mass composition in a human subject, the device comprising:
  - electrodes disposed in electrical contact with the subject's scalp at a location
  - 5 corresponding to each of the subject's left and right vestibular systems; and
  - a current source in electrical communication with the electrodes for applying galvanic vestibular stimulation (GVS) to the subject.
  
2. The device of claim 1, wherein the current source produces a constant
- 10 current within a predetermined voltage range.
  
3. The device of claim 2, wherein the current source produces a current having alternating polarity.
  
- 15 4. The device of claim 1, wherein the current source further comprises a feedback loop for measuring a resistance across the subject's scalp and adjusting a voltage output to maintain a constant current across the subject's scalp.
  
5. The device of claim 1, wherein the current source produces a current within
- 20 a range of 0.001 mA to 5 mA.
  
6. The device of claim 1, wherein the current source includes a controller, and further comprises:
  - an external sensor for detecting a condition of the subject and generating a
  - 25 signal corresponding to the detected condition;
  - a communication device for inputting the sensor signal to the device;
  - wherein the controller adjusts a characteristic of the GVS in response to the detected condition.
  
- 30 7. The device of claim 6, wherein the external sensor is a heart rate monitor and the characteristic of the GVS that is adjusted in response to the sensor signal is frequency.

8. The device of claim 6, wherein the communication device is a wireless transmitter/receiver.

9. The device of claim 6, wherein the external sensor is a position or motion  
5 sensor

10. The device of claim 1, wherein the current source produces a sinusoidal current having a frequency that is less than the subject's cardiac frequency.

10 11. A method for altering body mass composition in a human subject, the method comprising:  
applying galvanic vestibular stimulation (GVS) to the subject.

12. The method of claim 11, wherein the GVS is applied by disposing an  
15 electrode on the subject's scalp proximate to each mastoid process.

13. The method of claim 11, wherein the GVS comprises a current having a constant level and an alternating polarity.

20 14. The method of claim 13, wherein the constant current level is maintained by a feedback loop adapted to measure a resistance across the subject's scalp and adjust a voltage output to maintain the current level.

15. The method of claim 11, wherein the GVS comprises a sinusoidal current  
25 having a frequency that is less than the subject's cardiac frequency.

16. The method of claim 11, wherein the GVS is applied for a predetermined period of time at a regular interval.

30 17. The method of claim 16, wherein the regular interval is daily, weekly, or a combination thereof.

-30-

18. The method of claim 11, wherein the GVS is adjusted in response to input from an external sensor.

19. The method of claim 18, wherein the external sensor is a heart rate  
5 monitor.

20. A method of decreasing total body fat in a human subject in need thereof comprising:

10 applying galvanic vestibular stimulation (GVS) to the subject.

21. The method of claim 20, wherein the GVS is applied by disposing an electrode on the subject's scalp proximate to each mastoid process.

22. The method of claim 20, wherein the GVS comprises a current having a  
15 constant level and an alternating polarity.

23. The method of claim 22, wherein the constant current level is maintained by a feedback loop adapted to measure a resistance across the subject's scalp and adjust a voltage output to maintain the current level.  
20

24. The method of claim 20, wherein the GVS comprises a sinusoidal current having a frequency that is less than the subject's cardiac frequency.

25. The method of claim 20, wherein GVS is applied for a predetermined  
25 period of time at a regular interval.

26. The method of claim 25, wherein the regular interval is daily, weekly, or a combination thereof.

30 27. The method of claim 20, wherein the GVS is adjusted in response to input from an external sensor.

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28. The method of claim 27, wherein the external sensor is a heart rate monitor.

29. A method of increasing relative percentage lean muscle mass in a human  
5 subject in need thereof comprising:  
applying galvanic vestibular stimulation (GVS) to the subject.

30. The method of claim 29, wherein the GVS is applied by disposing an  
electrode on the subject's scalp proximate to each mastoid process.  
10

31. The method of claim 29, wherein the GVS comprises a current having a  
constant level and an alternating polarity.

32. The method of claim 31, wherein the constant current level is maintained  
15 by a feedback loop adapted to measure a resistance across the subject's scalp and  
adjust a voltage output to maintain the current level.

33. The method of claim 29, wherein the GVS comprises a sinusoidal current  
having a frequency that is less than the subject's cardiac frequency.  
20

34. The method of claim 29, wherein GVS is applied for a predetermined  
period of time at a regular interval.

35. The method of claim 34, wherein the regular interval is daily, weekly, or a  
25 combination thereof.

36. The method of claim 29, wherein the GVS is adjusted in response to input  
from an external sensor.

30 37. The method of claim 36, wherein the external sensor is a heart rate  
monitor.

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38. A method of increasing bone mineral density in a human subject in need thereof comprising:

applying galvanic vestibular stimulation (GVS) to the subject.

5           39. The method of claim 38, wherein the GVS is applied by disposing an electrode on the subject's scalp proximate to each mastoid process.

40. The method of claim 38, wherein the GVS comprises a current having a constant level and an alternating polarity.

10

41. The method of claim 40, wherein the constant current level is maintained by a feedback loop adapted to measure a resistance across the subject's scalp and adjust a voltage output to maintain the current level.

15           42. The method of claim 38, wherein the GVS comprises a sinusoidal current having a frequency that is less than the subject's cardiac frequency.

43. The method of claim 38, wherein GVS is applied for a predetermined period of time at a regular interval.

20

44. The method of claim 43, wherein the regular interval is daily, weekly, or a combination thereof.

25           45. The method of claim 38, wherein the GVS is adjusted in response to input from an external sensor.

46. The method of claim 45, wherein the external sensor is a heart rate monitor.

30

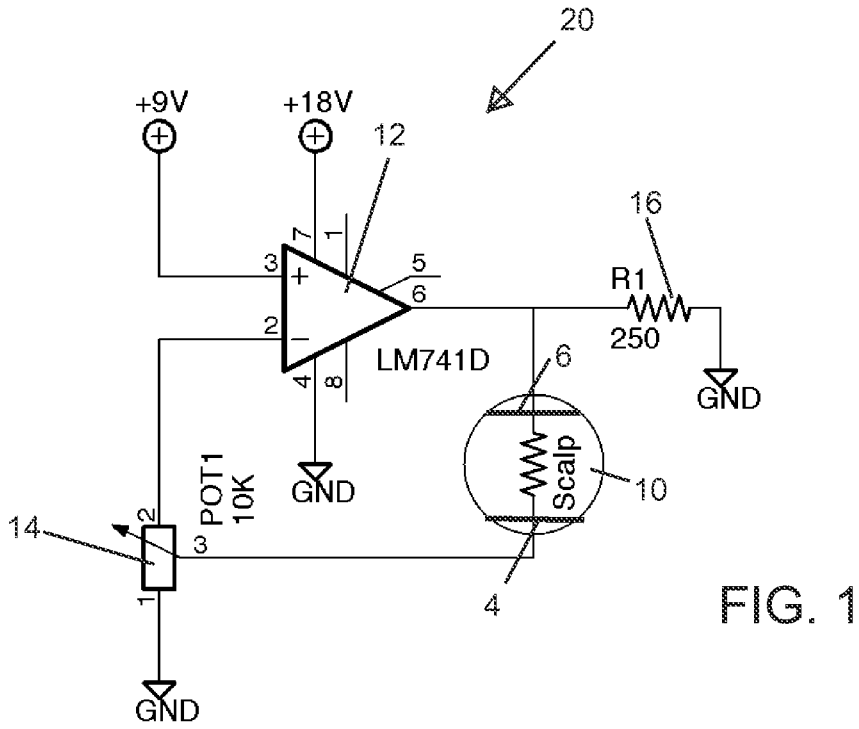


FIG. 1

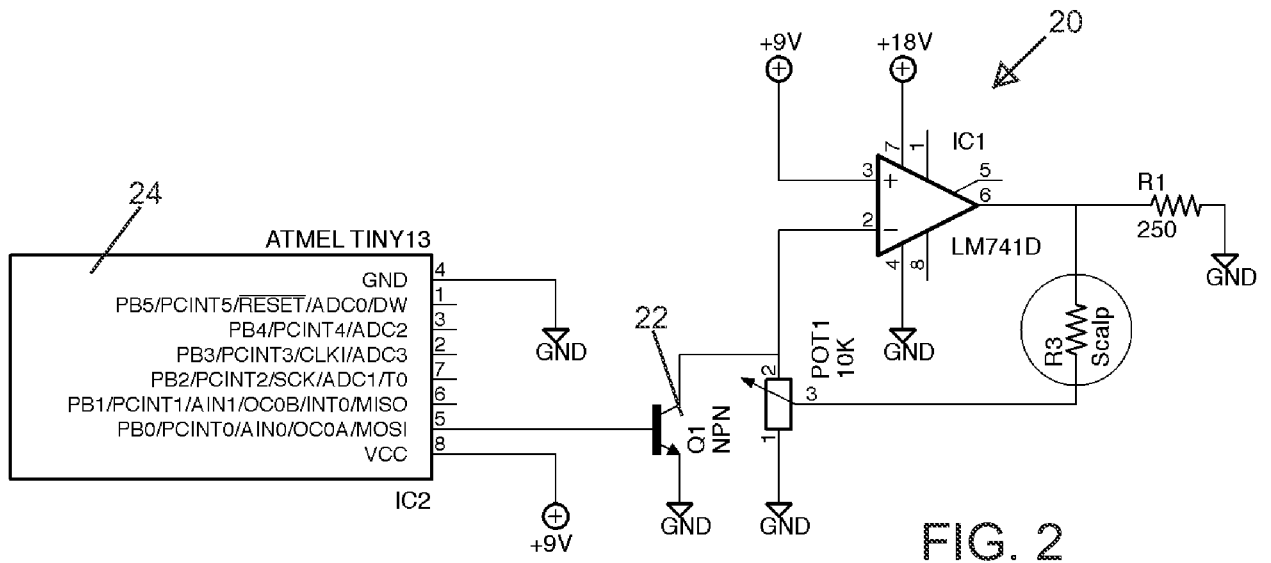


FIG. 2

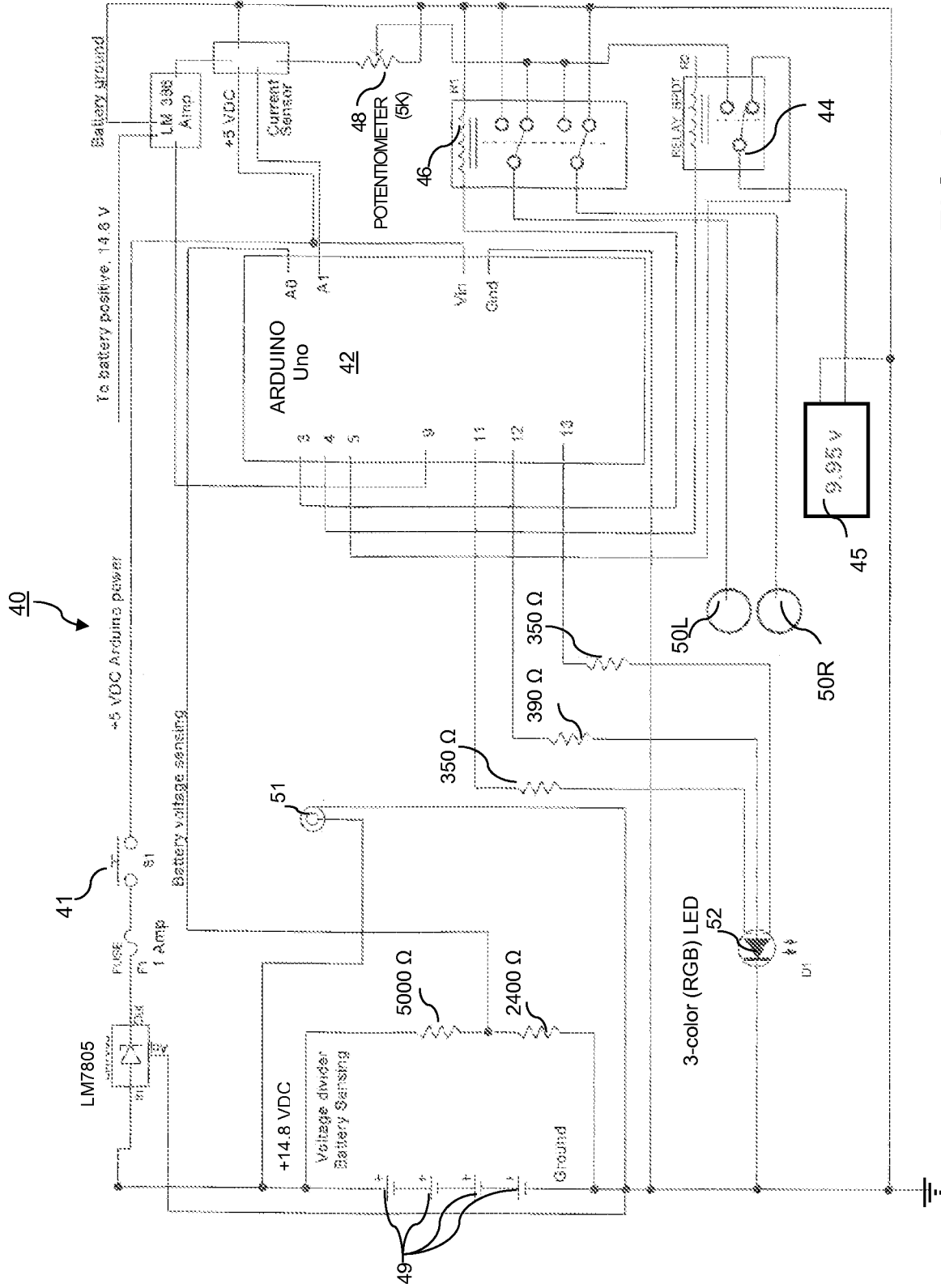


FIG. 3

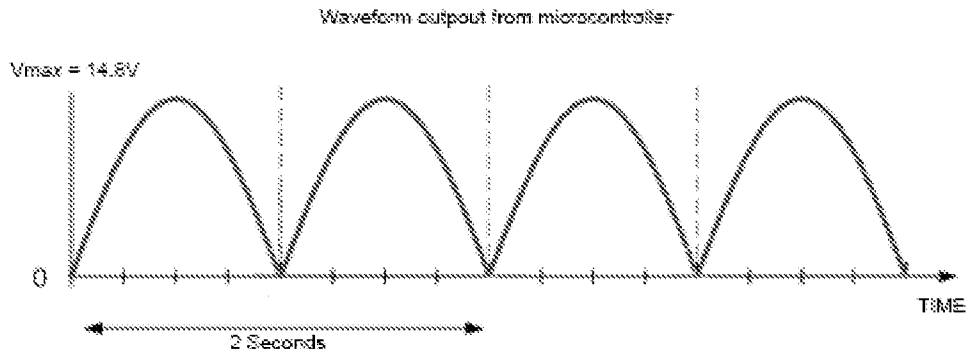


FIG. 4A

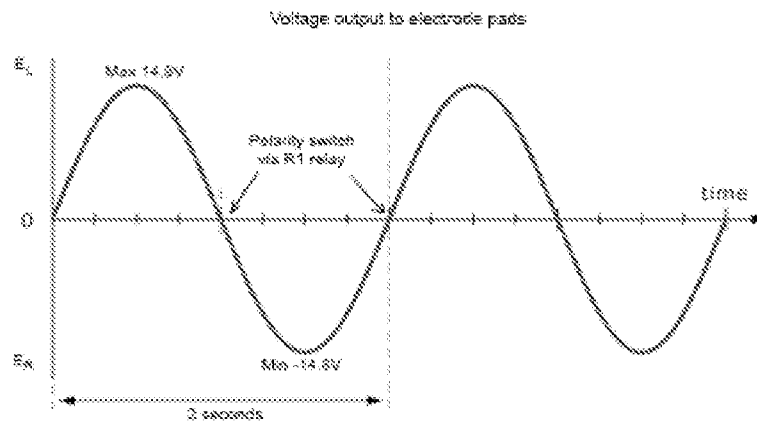
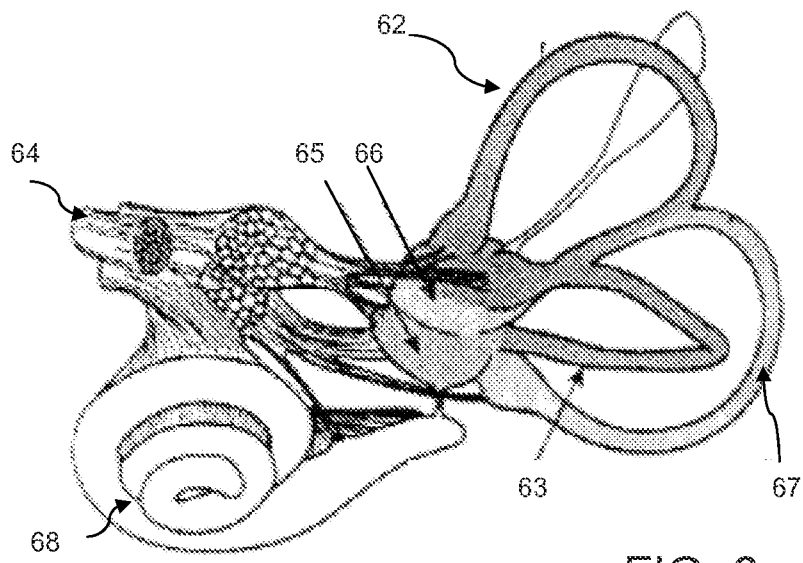
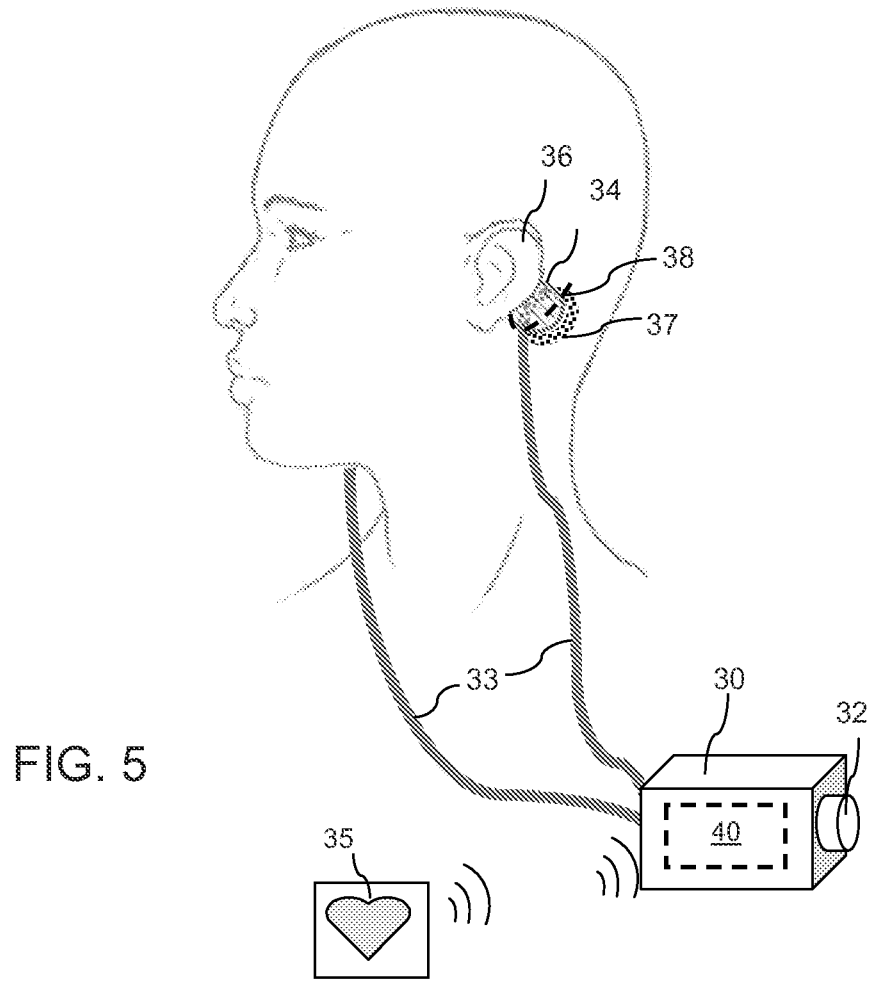


FIG. 4B



Name: XXXXXXXXXXXXXXXX	Gender: Female	Height: 160.4 cm
Patient ID: XXXXXXXXXXXX	Ethnicity: Hispanic	Weight: 84.4 kg
DOB: XX-XX-1989		Age: 23

**Scan Information:**

Scan Date: 10-08-2012  
 Scan Type: Whole body  
 Analysis: October 08, 2012 13:53  
 Version 12.7.3.1  
 Auto Whole Body  
 Operator: CK  
 Model: Discovery W (S/N 82084)  
 Comment:

**DXA Results Summary**

Region	BMC (g)	Fat (g)	Lean (g)	Lean + BMC (g)	Total Mass (g)	% Fat
L Arm	118.37	2120.2	2189.7	2308.0	4428.2	47.9
R Arm	135.21	2028.4	2773.0	2908.2	4936.6	41.1
Trunk	462.70	19364.9	23881.9	24344.6	43710.4	44.3
L Leg	321.72	4481.8	7261.1	7582.8	12064.6	37.1
R Leg	325.62	3965.0	8388.8	8714.4	12679.4	31.3
Subtotal	1363.62	31961.1	44494.5	45858.1	77819.2	41.1
Head	454.0	986.3	3487.2	3941.2	4927.5	20.0
<b>Total</b>	<b>1817.62</b>	<b>32947.4</b>	<b>47981.7</b>	<b>49799.3</b>	<b>82746.7</b>	<b>39.8</b>

FIG. 7

Name: XXXXXXXXXXXXXXXX  
 Patient ID: XXXXXXXXXXXX  
 DOB: XX-XX-1989

Gender: Female  
 Ethnicity: Hispanic

Height: 160.4 cm  
 Weight: 84.4 kg  
 Age: 23

**Scan Information:**

Scan Date: 12-07-2012  
 Scan Type: Whole body  
 Analysis: December 07, 2012 09:40  
 Version 12.7.3.1  
 Auto Whole Body  
 Operator: CK  
 Model: Discovery W (S/N 82084)  
 Comment:

**DXA Results Summary**

<b>Region</b>	<b>BMC (g)</b>	<b>Fat (g)</b>	<b>Lean (g)</b>	<b>Lean + BMC (g)</b>	<b>Total Mass (g)</b>	<b>% Fat</b>
L Arm	108.9	1989.4	2440.2	2549.1	4538.5	43.8
R Arm	136.75	1999.0	2990.0	3127.7	5126.7	39.0
Trunk	470.80	18941.8	25134.3	25605.1	44546.9	42.5
L Leg	311.24	4003.6	7632.6	7943.9	11947.5	33.5
R Leg	342.31	3950.1	8430.3	8772.6	12722.8	31.0
Subtotal	1370.00	30883.9	46628.4	47998.4	78882.3	39.2
Head	450.22	956.0	3441.8	3892.0	4848.0	19.7
<b>Total</b>	<b>1820.22</b>	<b>31839.9</b>	<b>50070.1</b>	<b>51890.4</b>	<b>83730.3</b>	<b>38.0</b>

**FIG. 8**

INTERNATIONAL SEARCH REPORT

International application No.  
PCT/US2014/019658

**A. CLASSIFICATION OF SUBJECT MATTER**  
 IPC(8) - A61N 1/18 (2014.01)  
 USPC - 607/148  
 According to International Patent Classification (IPC) or to both national classification and IPC

**B. FIELDS SEARCHED**

Minimum documentation searched (classification system followed by classification symbols)  
 IPC(8) - A61N 1/18, 1/20, 1/32, 1/36 (2014.01)  
 USPC - 607/all, 2, 62, 75, 115, 139, 148

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched  
 CPC - A61N 1/18, 1/20, 1/32, 1/36 (2014.02)

Electronic data base consulted during the international search (name of data base and, where practicable, search terms used)  
 Orbit, Google Patents, Google Scholar,

**C. DOCUMENTS CONSIDERED TO BE RELEVANT**

Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X	US 6,219,578 B1 (COLLINS et al) 17 April 2001 (17.04.2001) entire document	1-3,5-6,9,11-13,16-18,20-22,25-27,29-31,34-36,38-40,43-45
Y		4, 7-8, 10, 14-15, 19, 23-24,28,32-33,37,41-42, 46
Y	US 2009/0082831 A1 (PAUL et al) 26 March 2009 (26.03.2009) entire document	4, 7-8, 10, 14-15, 19, 23-24,28,32-33,37,41-42, 46
A	US 8,041,429 B2 (KIRBY) 18 October 2011 (18.10.2011) entire document	1-46
A	US 2009/0182399 A1 (SYLVESTRE) 16 July 2009 (16.07.2009) entire document	1-46

Further documents are listed in the continuation of Box C.

\* Special categories of cited documents:  
 "A" document defining the general state of the art which is not considered to be of particular relevance  
 "E" earlier application or patent but published on or after the international filing date  
 "L" document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified)  
 "O" document referring to an oral disclosure, use, exhibition or other means  
 "P" document published prior to the international filing date but later than the priority date claimed  
 "T" later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention  
 "X" document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone  
 "Y" document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art  
 "&" document member of the same patent family

Date of the actual completion of the international search 23 May 2014	Date of mailing of the international search report 06 JUN 2014
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Name and mailing address of the ISA/US Mail Stop PCT, Attn: ISA/US, Commissioner for Patents P.O. Box 1450, Alexandria, Virginia 22313-1450 Facsimile No. 571-273-3201	Authorized officer: Blaine R. Copenheaver PCT Helpdesk: 571-272-4300 PCT OSP: 571-272-7774
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专利名称(译)	使用电流前庭刺激改变体重组成的方法和系统		
公开(公告)号	<a href="#">EP2961474A4</a>	公开(公告)日	2016-10-19
申请号	EP2014757548	申请日	2014-02-28
[标]申请(专利权)人(译)	加利福尼亚大学董事会		
申请(专利权)人(译)	加利福尼亚大学董事会		
当前申请(专利权)人(译)	加利福尼亚大学董事会		
[标]发明人	MCGEOCH PAUL DUNCAN RAMACHANDRAN VILAYANUR S		
发明人	MCGEOCH, PAUL DUNCAN RAMACHANDRAN, VILAYANUR S.		
IPC分类号	A61N1/18 A61N1/36 A61B5/00 A61B5/053 A61N1/04 A61N1/05		
CPC分类号	A61B5/0531 A61B5/0537 A61B5/4836 A61B5/4872 A61N1/0456 A61N1/0526 A61N1/36031 A61N1/36034 A61N1/36036 A61N1/37211 A61N1/0408 A61N1/36014		
代理机构(译)	HART , DEBORAH MARY		
优先权	61/771766 2013-03-01 US		
其他公开文献	EP2961474A1		
外部链接	<a href="#">Espacenet</a>		

#### 摘要(译)

提供了一种用于通过使用电极放置成在对应于受试者的左前庭系统和右前庭系统中的每一个的位置处与受试者的头皮电接触的电极来改变人类受试者的体重组成的装置和方法。电流源包括用于测量受试者的头皮上的电阻并调节电压输出以维持受试者的头皮上的恒定电流的反馈回路。GVS可以以规则的间隔应用预定时间段。