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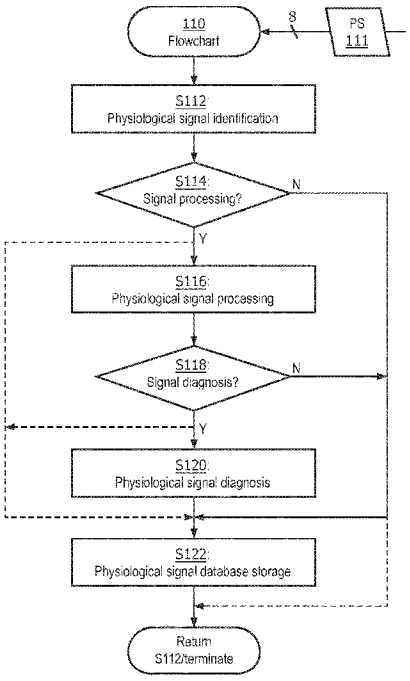

FIG. 3

(57) Abstract: A central signal segregation station (100) employs a signal acquisition controller (103) and a signal segregation controller (104). In operation, the signal acquisition controller (103) receives a plurality of different types of physiological signals from a plurality of unknown physiological sensors (10; 20; 30; 40; 50; 60; 70; 80). For a monitoring of the physiological signals, the signal segregation controller (104) identifies a particular type of each physiological signal based on distinct signal features of each physiological signal corresponding to a different physiological signal model (101) among a plurality of physiological signal models (101) derived from known types of physiological sensors. For analyzing the physiological signals, the station (100) may further employ a signal analyzing controller (105) executing signal quality processing of the physiological signals, providing signal-specific feedback to any physiological sensor(s) communicating low quality physiological signal(s), annotating specific regions of each physiological signal having maximum diagnostic information and/or performing a confirmatory diagnosis of the physiological signals.

WO 2018/011297 A1

CENTRAL SIGNAL SEGREGATION SYSTEM

TECHNICAL FIELD

Various embodiments of the present disclosure generally relate to central monitoring systems and more particularly, but not exclusively, relates to central monitoring systems for monitoring and analyzing signals representative of human physiological activity (*e.g.*, cardiovascular, respiratory, skin physiology, *etc.*).

BACKGROUND

An outpatient, as used herein, is a patient who is not hospitalized overnight after visiting a healthcare facility (*e.g.*, a hospital, a clinic, *etc.*) for a diagnosis and/or a treatment of an unhealthy condition. Mobile physiological sensors as known in the art of the present disclosure provide an efficient, accurate and economic method for monitoring a health of outpatients, particularly for supporting energy expedition calculations of outpatients.

Examples of such mobile physiological sensors include, but are not limited to, electrocardiogram ("ECG") monitors, respiration electrode patches, pulse oximeters, blood pressure monitors, galvanic skin response sensors, skin temperature sensors, heat flux sensors and near body temperature sensors. Future mobile physiological sensors may include, but not be limited to, arterial blood gas sensors, electroencephalography ("EEC") sensors and electromyogram ("EMG") sensors.

A central monitoring station, as the term is used herein,implements a communication protocol for exchanging information with remote sensors like mobile physiological sensors. A communication protocol standard of particular relevance in the domain of a physicological signal monitoring and analyzing by a central monitoring station is the global ISO/IEEE 11073 Personal Health Device (PHD) Communication family of standards. Current implementions of this family of standards involve the exchange of source identifying information of a mobile physiological sensor whereby a central montioring station knows the type of physiologal signal being communicated by the mobile physicological sensor. More particularly, an encrypted payload may be sent by the mobile physiological sensor across a communication channel established between the mobile physiological sensor and the central monitoring station whereby the payload includes bit information explicitly mapping the mobile physiological sensor

and whereby the central monitorting station decrypts and deciphers the bit informaiton to identify the type of physiologal signal being communicated by the mobile physicological sensor. This dependency by the central monitoring station of source identifying information of the physiological sensor facilitates an applicable montioring and analyzing of the physiological signal by the central monitoring station.

For example, FIG. 1 illustrates a central electrocardiogram ("ECG") monitoring station 12 for exchanging information with eight (8) ECG monitors 10. Central ECG monitoring station 12 and ECG montiors 10 implement a communication protocol (*e.g.*, the ISO/IEEE 11073-20601 bi-directional communication protocol) involving the exchange of source identifying information of ECG monitors 10 via playloads explicitly mapping ECG monitors 10 on a procotocol layer (*e.g.*, a transport layer) to thereby prepare central ECG monitoring station 12 and ECG montiors 10 for application layer messaging of ECG signals 11 from ECG monitors 10 to station 12. This dependency by ECG central monitoring station 12 of source identifying information of ECG monitors 10 facilitates applicable montioring and analyzing of ECG signals 11 via workstations 13 of central ECG monitoring station 12 (*e.g.*, a normality/abnormality interpretation of ECG signals 11).

A variety in the types of mobile physological sensors has been increasing in view of an ever increasing poplultion of outpatient requiring long-term care due to a rising average life expectancy, a higher ratio of seniors among the general population and an increased prevalence of chornic diseseaes. With the increasing varitey of types of mobile physiolocial sensors entering the healthcare market, there is a need for a central monitoring station having an independency on physiological sensor identifying information for signal monitoring and/or analysis.

SUMMARY

To improve upon the advantages and benefits of central monitoring stations for monitoring and/or analyzing one or more physiological signals, the present disclosure provides systems, stations, controllers and methods premised on an implementation of an independency of physiological sensor identifying information for signal monitoring and/or analysis of physicological signals, particularly physiological signals generated by varied types of physiological sensors.

For purposes of the present disclosure, the term "central monitoring station" broadly encompasses all central monitoring stations, known prior to the present disclosure, having a dependency on physiological sensor identifying information for monitoring and/or analyzing one or more types of physiological signals (*e.g.*, a need for payload bit informaitoin explicitily mapping physiological sensors generated the physiolgoical signals). Examples of such central montioring stations include, but are not limited to, the IntelliVue Information Center iX (PIIC).

Also for purposes of the present disclosure, the term "central signal segregation station" broadly encompasses a central monitoring station having a structural configuration incorporating inventive principles of the present disclosure as exemplary described herein for implementing an independency of physiological sensor identifying information for signal monitoring and/or analysis of a plurality of physiological signals, particularly physiological signals generated by varied types of physiological sensors, and the term "central signal segregation method" broadly encompasses all methods that incorporate the inventive principles of the present disclosure as exemplary described herein for implementing an independency of physiological sensor identifying information for signal monitoring and/or analysis of physiological signals by a central signal segregation station.

Various embodiments described herein include a central signal segregation station employing a signal acquisition controller and a signal segregation controller. In operation, the signal acquisition controller receives a plurality of different types of physiological signals from a plurality of unknown physiological sensors (*e.g.*, electrocardiogram ("ECG") monitors, respiration electrode patches, pulse oximeters, blood pressure monitors, galvanic skin response sensors, skin temperature sensors, heat flux sensors and near body temperature sensors).

For a monitoring of the physiological signals, the signal segregation controller identifies a particular type of each physiological signal based on distinct signal features of each physiological signal corresponding to a different physiological signal model among a plurality of physiological signal models derived from known types of physiological sensors. The distinct signal features of each physiological signal established an independency by the signal segregation controller of physiological sensor identifying information for signal monitoring and/or analysis of the

physiological signals (*e.g.*, the signal segregation controller identifies each physiological signal without any assistance or need for payload bit information explicitly mapping physiological sensors generated the physiological signals).

For an analysis of the identified physiological signals with or without monitoring, the central signal segregation station may further employ a signal analyzing controller. If employed, subsequent to the type identification of each physiological signal by the signal segregation controller, the signal analyzing controller may further:

(1) execute signal quality processing of the physiological signals (*e.g.*, a signal-to-noise quality measurement);

(2) provide signal-specific feedback to any physiological sensor(s) communicating low quality physiological signal(s);

(3) annotate specific regions of each high quality physiological signal having maximum diagnostic information; and/or

(4) perform an auto confirmatory diagnosis of each high quality physiological signal, particularly in view of context aware information appended to a physiological signal (*e.g.*, a geolocation and any accelerated motion of a physiological sensor).

Various embodiments described herein include a central signal segregation system employing a plurality of unknown physiological sensors and a central signal segregation station. In operation, each unknown physiological sensor transmits a different type of physiological signals to the central signal segregation station (*e.g.*, electrocardiogram ("ECG") signal, a respiration signal $1/\Omega_R$, an oxygen saturation signal SO_2, a blood pressure signal (systolic/diastolic), a galvanic skin response signal $1/\Omega_S$, a skin temperature signal °F/°C, a heat flux signal W/m^2 and a near body temperature signal °F/°C).

For a monitoring of the physiological signals, the central signal segregation station identifies a particular type of each physiological signal based on distinct signal

features of each physiological signal corresponding to a different physiological signal model among a plurality of physiological signal models derived from known types of physiological sensors. The distinct signal features of each physiological signal established an independency by the signal segregation controller of physiological sensor identifying information for signal monitoring and/or analysis of the physiological signals (*e.g.*, the signal segregation controller identifies each physiological signal without any assistance or need for payload bit information explicitly mapping physiological sensors generated the physiological signals).

For an analysis of the identified physiological signals with or without monitoring, the central signal segregation station may further:

(1) execute signal quality processing of the physiological signals (*e.g.*, a signal-to-noise quality measurement);

(2) provide signal-specific feedback to any physiological sensor(s) communicating low quality physiological signal(s);

(3) annotate specific regions of each high quality physiological signal having maximum diagnostic information; and/or

(4) perform a confirmatory diagnosis of each high quality physiological signals particularly in view of context aware information appended to a physiological signal (*e.g.*, a geolocation and any accelerated motion of a physiological sensor).

Various embodiments described herein include a central signal segregation method involving a central signal segregation station receiving a plurality of different types of physiological signals from a plurality of unknown physiological sensors (*e.g.*, electrocardiogram ("ECG") monitors, respiration electrode patches, pulse oximeters, blood pressure monitors, galvanic skin response sensors, skin temperature sensors, heat flux sensors and near body temperature sensors).

For a monitoring of the physiological signals, the central signal segregation method further involves the central signal segregation station identifying the type of each physiological signal based on distinct signal features of each physiological signal corresponding to a different physiological signal model among a plurality of physiological signal models derived from known types of physiological sensors. The distinct signal features of each physiological signal established an independency by the signal segregation controller of physiological sensor identifying information for signal monitoring and/or analysis of the physiological signals (*e.g.*, the signal segregation controller identifies each physiological signal without any assistance or need for payload bit information explicitly mapping physiological sensors generated the physiological signals).

For an analysis of the identified physiological signals with or without monitoring, the central signal segregation method may further involve the central signal segregation station:

(1) executing signal quality processing of the physiological signals (*e.g.*, a signal-to-noise quality measurement);

(2) providing signal-specific feedback to any physiological sensor(s) communicating low quality physiological signal(s);

(3) annotating specific regions of each high quality physiological signal having maximum diagnostic information; and/or

(4) performing a confirmatory diagnosis of each high quality physiological signal, particularly in view of context aware information appended to the physiological signal (*e.g.*, a geolocation and any accelerated motion of a physiological sensor).

For purposes of the present disclosure,

(1) terms of the art including, but not limited to, "physiological sensor", "monitoring", "analyzing" and "diagnosing" are to be interpreted as understood in the art of the present disclosure and as exemplary described herein;

(2) the phrase "unknown physiological sensors" broadly encompasses mobile and immobile physiological sensors excluding source identifying information within a communication protocol implemented by the physiological sensors;

(3) the term "physiological signal model" broadly encompasses all models for estimating a probability of a particular type of a physiological signal based on one or more signal features of the physiological signal. An example of a physiological signal model includes machine learning methods (*e.g.*, supervised, unsupervised and semi-supervised), but is not limited to, a logistic regression model, a linear regression model, a support vector machine model, a classification model, a clustering model, a dimensionality reduction model, an association rule learning model and a decision tree model;

(4) the term "signal features" broadly encompasses any and all distinctive features of a physiological signal facilitating an identification of the physiological signal. Examples of such signal features include, but are not limited to:

(a) a resistive index;

(b) a pulsatility index;

(c) a relative acceleration time;

(d) a relative decay time;

(e) a flow acceleration;

(f) a constant flow ratio;

(g) a height width index;

(h) a peak to peak pulsatility index;

(i) a bandwidth index;

(j) an envelope roll-off;

(k) a higher order statistics;

(l) an envelope centroid;

(m) an average rising slope;

(n) a spectral broadening ratio; and

(o) a profile shape;

(5) the term "low quality" broadly encompasses any qualitative nature of a physiological signal impeding an analysis of the physiological signal, and the term "high quality" broadly encompasses a qualitative nature of a physiological signal suitable for an analysis of the physiological signal;

(6) the term "context aware information" broadly encompasses any information related to an operational and environment context within which a physiological sensor is generating a physiological signal. Examples of context aware information include, but are not limited to, a geolocation, a temperature, a light flux, a noise level and an accelerated motion of a physiological sensor.

(7) the term "controller" broadly encompasses all structural configurations of an application specific main board or an application specific integrated circuit housed within or linked to a central signal segregation station for controlling an application of various inventive principles of the present disclosure as subsequently described herein. The structural configuration of the controller may include, but is not limited to, processor(s), computer-usable/computer readable storage medium(s), an operating system, application module(s), peripheral device controller(s), slot(s) and port(s). Any descriptive labeling of a controller herein (*e.g.*, "signal acquisition", and "signal segregation") serves to identify a controller as described and claimed herein without specifying or implying any additional limitation to the term "controller";

(8) the term "application module" broadly encompasses a component of a controller consisting of an electronic circuit and/or an executable program (*e.g.*, executable software and/or firmware stored on non-transitory computer readable medium(s)) for executing a specific application. Any descriptive labeling of an application module herein (*e.g.*, a "signal acquisition module", "signal source identifier", "signal quality manager", "annotation manager", "diagnostic analyzer" and "database manager ") serves to identify a particular application module as described and claimed herein without specifying or implying any additional limitation to the term "application module"; and

(9) the terms "signal" and "data" broadly encompasses all forms of a detectable physical quantity or impulse (*e.g.*, voltage, current, *etc.*) as understood in the art of the present disclosure and as exemplary described herein for transmitting information in support of applying various inventive principles of the present disclosure

as subsequently described herein. Any descriptive labeling for the terms "signal" and "data" herein facilitates a distinction between signals as described and claimed herein without specifying or implying any additional limitation to the terms "signal" and "data".

The foregoing forms and other forms of the inventions of the present disclosure as well as various features and advantages of the inventions of the present disclosure will become further apparent from the following detailed description of various embodiments of the inventions of the present disclosure read in conjunction with the accompanying drawings. The detailed description and drawings are merely illustrative of the inventions of the present disclosure rather than limiting, the scope of the present inventions of the present disclosure being defined by the appended claims and equivalents thereof.

BRIEF DESCRIPTION OF THE DRAWINGS

FIG. 1 illustrates an exemplary embodiment of a central ECG monitoring system as known in the art;

FIG. 2 illustrates an exemplary embodiment of a central signal segregation system in accordance with the inventive principles of the present disclosure;

FIG. 3 illustrates a flowchart representative of an exemplary embodiment of a central signal segregation method in accordance with the inventive principles of the present disclosure.

FIG. 4 illustrate an exemplary embodiment of a central signal segregation station in accordance with the inventive principles of the present disclosure.

FIG. 5A illustrates an exemplary embodiment of a signal segregation controller in accordance with the inventive principles of the present disclosure.

FIG. 5B illustrates an exemplary embodiment of a signal analyzing controller in accordance with the inventive principles of the present disclosure.

FIGS. 6A and 6B illustrate an exemplary embodiment of a signal source identifier in accordance with the inventive principles of the present disclosure.

FIG. 7 illustrates an exemplary embodiment of a signal quality manager in accordance with the inventive principles of the present disclosure.

FIG. 8 illustrates an exemplary embodiment of an annotation manager in accordance with the inventive principles of the present disclosure.

FIG. 9 illustrates an exemplary embodiment of a diagnostic analyzer in accordance with the inventive principles of the present disclosure.

DETAILED DESCRIPTION

To facilitate an understanding of the embodiments of the present disclosure, the following description of FIGS. 2 and 3 teaches inventive principles of central signal segregation systems and central signal segregation methods of the present disclosure. While the description of FIGS. 2 and 3 are provided in the context of a plurality of mobile physiological sensors including an electrocardiogram ("ECG") monitor, a respiration electrode patch, a pulse oximeter, a blood pressure monitor, a galvanic skin response sensor, a skin temperature sensor, a heat flux sensor and a near body temperature sensor, those having ordinary skill in the art of the present disclosure will appreciate how to apply the inventive principles of the present disclosure to make and use a variety of central signal segregation systems and central signal segregation methods of the present disclosure in the context of numerous physiological sensors as shown and of additional physiological sensors, mobile and/or immobile.

Referring to FIG. 2, one embodiment of a central signal segregation system of the present disclosure employs, as known in the art of the present disclosure, a plurality of physiological sensors including:

1. an ECG monitor 10 generating an ECG signal 11;
2. a respiration electrode patch 20 generating a respiration signal 21;
3. a pulse oximeter 30 generating an oxygen saturation signal 31;
4. a blood pressure monitor generating a blood pressure signal 41;
5. a galvanic skin response sensor 50 generating a galvanic skin response signal 51;
6. a skin temperature sensor 60 generating a skin temperature signal 61;
7. a heat flux sensor 70 generating a heat flux signal 71, and
8. a near body temperature sensor 80 generating a near body temperature signal 81.

Still referring to FIG. 2, the physiological sensors transmit the physiological signals via a network 90 (*e.g.*, an intranet or an internet) to a central signal segregation

station 100 as shown. As will be understood, the central signal segregation station may be implemented in various hardware arrangements such as a stand-alone server or as one or more virtual machines hosted on hardware in a cloud computing environment or distributed among multiple cloud computing environments. In practice, the physiological sensors may be sequentially or concurrently transmitting a subset or an entire set of the physiological signals, and two or more of the physiological sensors may be monitoring the same individual outpatient.

Also in practice, the physiological sensors and central signal segregation station 100 implement a communication protocol (*e.g.*, the ISO/IEEE 11073-20601 bi-directional communication protocol) excluding the exchange of source identifying information of the physiological sensors of any layer of the communication protocol (*e.g.*, excluding payload bit information explicitly mapping physiological sensors generated the physiological signals). To address this independency by central signal segregation station 100 of source identifying information of the "unknown" physiological sensors, central signal segregation station 100 identifies a particular type of each physiological signal based on distinct signal features of each physiological signal corresponding to a different physiological signal model among a plurality of physiological signal models 101 derived from the known types of the physiological sensors.

Physiological signal models 101 provide for an estimation of a probability of a particular type of a physiological signal based on one or more signal features of the physiological signal as will be further described herein. In the context of the unknown physiological sensors of FIG. 2, central signal segregation station 100 is trained to generate:

1. an ECG signal model derived from signal features of training ECG signals generated by numerous and/or various types of ECG monitors whereby the ECG signal model provides an estimation of a probability that any physiological signal received by central signal segregation station 100 is an ECG signal;

2. a respiration signal model derived from signal features of training respiration signals generated by numerous and/or various types of respiration electrode patches whereby the respiration signal model provides an estimation of a probability that any physiological signal received by central signal segregation station 100 is a respiration signal;

3. an oxygen saturation signal model derived from signal features of training oxygen saturation signals generated by numerous and/or various types of pulse oximeters whereby the oxygen saturation signal model provides an estimation of a probability that any physiological signal received by central signal segregation station 100 is an oxygen saturation signal;

4. a blood pressure signal model derived from signal features of training blood pressure signals generated by numerous and/or various types of blood press monitors whereby the blood pressure signal model provides an estimation of a probability that any physiological signal received by central signal segregation station 100 is a blood pressure signal;

5. a galvanic skin response signal model derived from signal features of training galvanic skin response signals generated by numerous and/or various types of galvanic skin response sensors whereby the galvanic skin response signal model provides an estimation of a probability that any physiological signal received by central signal segregation station 100 is a galvanic skin response signal;

6. a skin temperature signal model derived from signal features of training skin temperature signals generated by numerous and/or various types of skin temperature sensors whereby the skin temperature signal model provides an estimation of a probability that any physiological signal received by central signal segregation station 100 is a skin temperature signal;

7. a heat flux signal model derived from signal features of training heat flux signals generated by numerous and/or various types of heat flux sensors whereby the heat flux signal model provides an estimation of a probability that any physiological signal received by central signal segregation station 100 is a heat flux signal; and

8. a near body temperature signal model derived from signal features of training near body temperature signals generated by numerous and/or various types of near body temperature sensors whereby the near body temperature signal model provides an estimation of a probability that any physiological signal received by central signal segregation station 100 is a near body temperature signal.

From the type identification of the physiological signals, central signal segregation station 100 process the physiological signals via the application layers of the communication protocol and operators of central signal segregation station 100 may access monitoring application(s) via workstations 102 to thereby visually monitor the physiological signals.

Additionally, central signal segregation station 100 may execute analyzing application(s) that provide analytical information to the operators via workstations 102 and/or as feedback to the physiological sensors as will be further described herein.

Also, context aware information may be appended by the physiological sensors to the physiological signals in support of the analyzing application(s) of central signal segregation station 100 as will be further described herein.

More particularly, FIG. 3 illustrates a flowchart 110 representative of one embodiment of a central signal segregation method of the present disclosure executable by central signal segregation station 100 (FIG. 2).

Referring to FIGS. 2 and 3, central signal segregation station 100 executes flowchart 110 in responsive to a concurrent reception of physiological signals 111 from the unknown physiological sensors.

Specifically, a stage S112 of flowchart 110 encompasses central signal segregation station 100 identifying a particular type of each physiological signal based

on distinct signal features of each physiological signal corresponding to a particular physiological signal model among a plurality of physiological signal models 101 derived from the known types of the physiological sensors.

Upon completion of stage S112, if central signal segregation station 100 is not structurally configured for signal quality processing of the identified physiological signals (*e.g.*, a signal-to-noise quality measurement), then central signal segregation station 100 proceeds to a stage S122 of flowchart 110 to manage a stream storage of the physiological signals within a database for monitoring purposes.

Otherwise, if central signal segregation station 100 is structurally configured for signal quality processing of the identified physiological signals (*e.g.*, a signal-to-noise quality measurement), then central signal segregation station 100 proceeds to a stage S116 of flowchart 110 to execute signal quality processing of the identified physiological signals and provide signal-specific feedback to any physiological sensor(s) communicating low quality physiological signal(s) as will be further described herein.

Prior to proceeding to stage S116, central signal segregation station 100 may initiate stage S122 for a stream storage of the physiological signals within a database as symbolized by the dashed arrows for monitoring purposes.

Upon completion of stage S116, if central signal segregation station 100 is not structurally configured for signal-specific diagnostic analyzing of the identified physiological signals of high quality, then central signal segregation station 100 proceeds to stage S122 of flowchart 110 to manage a stream storage of the physiological signals within the database.

Otherwise, if central signal segregation station 100 is structurally configured for signal-specific diagnostic analyzing of the identified physiological signals of high quality, then central signal segregation station 100 proceeds to a stage S120 of flowchart 110 to annotate specific regions of each identified physiological signal of high quality having maximum diagnostic information, and/or to perform a confirmatory diagnosis of identified physiological signal of high quality, particularly in view of context aware information appended to the physiological signals (*e.g.*, a geolocation and any accelerated motion of a physiological sensor) as will be further described herein.

Prior to proceeding to stage S120, central signal segregation station 100 may initiate or continue stage S122 for a stream storage of the physiological signals and associated processing information within the database as symbolized by the dashed arrows for monitoring and analytical purposes.

Upon completion of stage S120, central signal segregation station 100 may initiate or continue stage S122 for a stream storage of the physiological signals and associated processing and diagnostic information within the database for monitoring and analytical purposes.

Flowchart 110 is executed by central signal segregation station 100 in sequential or overlapping cycles. Thus, at any time during flowchart 110 or upon completion of stage S122, central signal segregation station 100 returns to stage S112 to initiate a new cycle until such time flowchart 110 is terminated (*e.g.*, central signal segregation station 100 is powered down for maintenance and/or upgrade).

From the descriptions of FIGS. 2 and 3, those having ordinary skill in the art of the present disclosure will appreciate the implementation by central signal segregation station 100 (FIG. 2) and flowchart 110 (FIG. 3) of an independency of physiological sensor identifying information for signal monitoring and optional analysis of the physicological signals.

To facilitate a further understanding of the present disclosure, the following description of FIGS. 4-9 further teaches inventive principles of central signal segregation stations of the present disclosure. While the description of FIGS. 4-9 are provided in the context of the plurality of mobile physiological sensors shown in FIG. 2, those having ordinary skill in the art of the present disclosure will appreciate how to apply the inventive principles of the present disclosure to make and use a variety of central signal segregation stations of the present disclosure in the context of numerous physiological sensors as shown in FIG. 2 and of additional physiological sensors, mobile and/or immobile.

Referring to FIG. 4, a signal acquisition module 130 of the present disclosure is installed on each unknown physiological sensor and structurally configured to transmit an associated physiological signal 131 in accordance with a communication protocol exclusive of any physiological sensor identifying information. If an associated physiological sensor in practice incorporates devices for generating context aware

information 132 (*e.g.*, geolocation and accelerated motion of the physiological sensor), then a signal acquisition module 130 will append the context aware information 132 with the physiological signal 131. Alternatively, context aware information 132 may be derived from a mobile phone or any connected device to the subject.

Still referring to FIG. 4, an embodiment 100a of central signal segregation station 100 (FIG. 2) employs a signal acquisition controller 103, a signal segregation controller 104, a signal analyzing controller 105, and a database 106. In practice, controllers 103-105 may be segregated as shown, or partially or fully integrated. Also, in practice, database 106 may be segregated from controllers 103-105 as shown or integrated/distributed within one or more of controllers 103-105.

Signal acquisition controller 103 is structurally configured for receiving physiological signals 131 in accordance with the communication protocol exclusive of any physiological sensor identifying information (*e.g.*, excluding any payload bit information explicitly mapping the associated physiologic sensor). In practice, signal acquisition controller 103 controls transmitters, receivers and/or transceivers (not shown) of central signal segregation station 100 as known in the art for receiving physiological signals 131 in accordance with the communication protocol and provides physiological signals 131 to signal segregation controller 104.

Signal segregation controller 104 is structurally configured in accordance with the inventive principles of the present disclosure for executing stage 112 of flowchart 110 (FIG. 3) and for executing stage S122 of flowchart 110 (if applicable). In practice, signal segregation controller 104 is trained to generate physiological signal models 101 as previously described herein (FIG. 2) and to apply each received physiological signal 131 to each physiological signal model 101 to identify a particular type of each physiological signal 131.

In practice, any embodiment of signal segregation controller 104 will be dependent upon various operational factors as will be appreciated by those having ordinary skill in the art of the present disclosure including, but not limited to, a variance in the types of physiological signals to be monitored and/or analyzed.

Referring to FIG. 5A, one embodiment 104a of signal segregation controller 104 employs a signal source identifier 150 and a database manager 160.

Signal source identifier 150 is structurally configured in accordance with the inventive principles of the present disclosure to generate the physiological signal models 101 (FIG. 2) for an estimation of a probability of a particular type of each physiological signal 131 based on one or more signal features of physiological signal 131. In practice, signal source identifier 150 may generate physiological signal models in the form of a logistic regression model, a linear support vector machine model and/or a decision tree model involving an extraction of signal features including, but not limited to:

1. a resistive index;
2. a pulsatility index;
3. a relative acceleration time;
4. a relative decay time;
5. a flow acceleration;
6. a constant flow ratio;
7. a height width index;
8. a peak to peak pulsatility index;
9. a bandwidth index;
10. an envelope roll-off;
11. a higher order statistics;
12. an envelope centroid;
13. an average rising slope;
14. a spectral broadening ratio; and
15. a profile shape.

For example, in a training phase of signal source identifier 150, FIG. 6A illustrate a feature extraction 150a by signal source identifier 150 of training physiological signals 133a-133h in the form of feature vectors 151 being an *n*-dimensional vector of signal features (s), $n \geq 1$ or a vector loop. Signal source identifier 50 thereafter applies a machined learning device 152 (*e.g.*, a support vector machine) to each feature vector 151 for model building 150b of physiological signal models 153 whereby the signal features of a feature vector 151 serve as independent

variables of models 153 and the dependent variable provides a probability estimation of the corresponding training physiological signal 133.

By further example, in an identification phase of signal source identifier 150, FIG. 6B illustrate a feature extraction 150c by signal source identifier 150 of received physiological signals 133 in the form of a feature vector 154 being an n-dimensional vector of signal features(s), $n \geq 1$ or a vector loop. Signal source identifier 50 thereafter applies feature vector 154 to each physiological signal model 153 to obtain a similarity measurement 155 (*e.g.*, $0 \leq SM \leq 1$). Physiological signal 131 is deemed to correspond the physiological signal model 153 providing the higher similarity measurement 155. For example, upon sufficient training, if physiological signal 131 is an ECG signal, then similarity measurement 155(1) of ECG model 153(1) should have the highest similarity measurement among all similarity measurements 151.

Referring back to FIG. 4, signal analyzing controller 105 is structurally configured in accordance with the inventive principles of the present disclosure for executing stages S116-S122 of flowchart 110 (FIG. 3). In practice, signal analyzing controller 105 executes analyzing application(s) that provide analytical information and/or signal feedback to the user(s)/monitor(s) of the physiological sensor(s) and/or operator(s) of the central signal segregation station will be further described herein.

In practice, any embodiment of signal analyzing controller 105 will be dependent upon various operational factors as will be appreciated by those having ordinary skill in the art of the present disclosure including, but not limited to, any and all delineated analytical techniques to be applied to the physiological signals.

Referring to FIG. 5B, one embodiment 105a of signal analyzing controller 105 employs a signal quality manager 170, an annotation manager 180, a diagnostic analyzer 190 and a database manager 200.

Signal quality manager 160 is structurally configured to execute signal quality processing of the identified physiological signals and provides signal-specific feedback to any physiological sensor(s) communicating low quality physiological signal(s). In practice, signal quality manager 160 may detect a required signal-to-noise (SNR) for each identified physiological signal. Further, signal quality manager 160 may ascertain if all the relevant fiducial points, which are needed for diagnosis level prediction, are present in each identified physiological signal. Also, if the signal quality is poor, then

signal quality manager 160 tries to identify the source of degradation either due to, for example, a wrong placement, an electromagnetic interference and/or a device malfunctioning of the associated physiological sensor. Signal quality manager 160 provides the feedback to a user/monitor of the physiological sensor and/or an operator of central signal segregation station on the proper usage of the device/ modification within the device parameter for obtaining proper SNR.

For example, as shown with a data flow in FIG. 7, signal quality manager 160 executes a signal quality processing of a physiological signal 131 based on the associated similarly measurement 155 or other signal identifier to yield a high quality check 171 or a low quality feedback 172 for database storage. Examples of the signal quality processing include, but are not limited to, a signal-to-noise quality measurement 170b and a fiducial point detection 170c. If physiological signal 131 exhibits low quality (*e.g.* high signal-to-noise ratio, failure to detect fiducials, *etc.*), then signal quality manager 170 executes a signal degradation analysis 170d involving a communication of low quality feedback signal 172 informative of the low quality nature of the physiological signal 131 with or without an identification of a determined reason for the signal degradation.

Referring back to FIG. 5B, annotation manager 180 is structurally configured to annotate specific regions of each identified high quality physiological signal having maximum diagnostic information. In practice, after an identified physiological signal has been denoted as have appreciable quality by signal quality manager 170, annotation manager 180 identifies the relevant part of the signal for analysis.

More particularly, the present disclosure recognizes that continuous monitoring of a physiological signal provides repeated signal trends which typically may or may not have any significant diagnostic value. For example, for an ECG signal, when the trend is continuously monitored, the change in ST segment, or the periodic shift of fiducial locations are of primary importance for the analysis rather than entire signal. Annotation manager 180 therefore identifies the signal regions which are unique and carry potential information for the analysis using information gain and modelling approach. Also, if content information is received (*e.g.*, geolocation and any accelerated motion), annotation manager 80 further annotates the activity being performed during the signal acquisition with the diagnostic region(s).

For example, as shown in FIG. 8, if a quality check 171 is received for a physiological signal 131, annotation manager 180 executes a diagnostic region annotation 180a involving a delineation of diagnostic region(s) (*e.g.*, diagnostic region 131b) and non-diagnostic region(s) (*e.g.*, non-diagnostic regions 131a and 131c) of physiological signal 130 of a signal cycle. The exemplary diagnostic region 131b may be identified based on historical understanding of a diagnostic nature of physiological signal 131 and/or the predictive elements of the associated physiologic signal model. Annotation manager 181 generates a diagnostic region annotation 181 for database storage appended with, if applicable, content aware information 132 occurring during a diagnostic region 131b.

Referring back to FIG. 5B, diagnostic analyzer 190 is structurally configured to perform a diagnosis of an identified high quality physiological signal of based on the associated diagnostic region annotation(s), particularly in view of any context aware information appended to diagnostic region annotation(s). In practice, after an annotation of an identified high quality physiological signal, diagnostic analyzer 190 extracts a trend among the physiological signals to correlate an observation to auto diagnose any pertinent aliments whereby a personalized care plan may be pushed to a user/monitor of the physiological device and/or an operator of the central signal segregation station.

For example, as shown in FIG. 9, diagnostic analyzer 190 executes a trend diagnosis 190a of physiological signals 131 from an individual subject based on the associated diagnostic region annotations 181. Any trend identification will be informative of any pertinent aliments and diagnostic analyzer 190 within the context aware information whereby a personalize care plan (PCC) may be communicated to a user/monitor of the physiological device and/or an operator of the central signal segregation station.

Referring to FIGS. 2-9, those having ordinary skill in the art will appreciate numerous benefits of the various embodiments of the present disclosure including, but not limited to, an independency of physiological sensor identifying information for signal monitoring and/or analysis of physicological signals by central signal segreation stations and methods.

Furthermore, as one having ordinary skill in the art will appreciate in view of the teachings provided herein, features, elements, components, *etc.* described in the present disclosure/specification and/or depicted in the Figures may be implemented in various combinations of electronic components/circuitry, hardware, executable software and executable firmware and provide functions which may be combined in a single element or multiple elements. For example, the functions of the various features, elements, components, *etc.* shown/illustrated/depicted in the Figures can be provided through the use of dedicated hardware as well as hardware capable of executing software in association with appropriate software. When provided by a processor, the functions can be provided by a single dedicated processor, by a single shared processor, or by a plurality of individual processors, some of which can be shared and/or multiplexed. Moreover, explicit use of the term "processor" should not be construed to refer exclusively to hardware capable of executing software, and can implicitly include, without limitation, digital signal processor ("DSP") hardware, memory (*e.g.*, read only memory ("ROM") for storing software, random access memory ("RAM"), non-volatile storage, *etc.*) and virtually any means and/or machine (including hardware, software, firmware, circuitry, combinations thereof, *etc.*) which is capable of (and/or configurable) to perform and/or control a process. Further, the term "processor" will be understood to encompass various types of hardware such as microprocessors, field-programmable gate arrays (FPGAs), application-specific integrated circuits (ASICs), and other hardware capable of performing the functions described herein. Further, as used herein, the term "non-transitory medium" will be understood to encompass both volatile memories (*e.g.*, DRAM, SRAM, *etc.*) and nonvolatile memories (*e.g.*, flash, magnetic, and optical storage) but to exclude transitory signals.

Moreover, all statements herein reciting principles, aspects, and embodiments, as well as specific examples thereof, are intended to encompass both structural and functional equivalents thereof. Additionally, it is intended that such equivalents include both currently known equivalents as well as equivalents developed in the future (*e.g.*, any elements developed that can perform the same or substantially similar function, regardless of structure). Thus, for example, it will be appreciated by one having ordinary skill in the art in view of the teachings provided herein that any block diagrams presented herein can represent conceptual views of illustrative system

components and/or circuitry embodying the principles described herein. Similarly, one having ordinary skill in the art should appreciate in view of the teachings provided herein that any flow charts, flow diagrams and the like can represent various processes which can be substantially represented in computer readable storage media and so executed by a computer, processor or other device with processing capabilities, whether or not such computer or processor is explicitly shown.

Furthermore, exemplary embodiments of the present disclosure can take the form of a computer program product or application module accessible from a computer-usable and/or computer-readable storage medium providing program code and/or instructions for use by or in connection with, *e.g.*, a computer or any instruction execution system. In accordance with the present disclosure, a computer-usable or computer readable storage medium can be any apparatus that can, *e.g.*, include, store, communicate, propagate or transport the program for use by or in connection with the instruction execution system, apparatus or device. Such exemplary medium can be, *e.g.*, an electronic, magnetic, optical, electromagnetic, infrared or semiconductor system (or apparatus or device) or a propagation medium. Examples of a computer-readable medium include, *e.g.*, a semiconductor or solid state memory, magnetic tape, a removable computer diskette, a random access memory (RAM), a read-only memory (ROM), flash (drive), a rigid magnetic disk and an optical disk. Current examples of optical disks include compact disk – read only memory (CD-ROM), compact disk – read/write (CD-R/W) and DVD. Further, it should be understood that any new computer-readable medium which may hereafter be developed should also be considered as computer-readable medium as may be used or referred to in accordance with exemplary embodiments of the present disclosure and disclosure.

Having described preferred and exemplary embodiments of novel and inventive central signal segregation stations, controllers and methods, (which embodiments are intended to be illustrative and not limiting), it is noted that modifications and variations can be made by persons having ordinary skill in the art in light of the teachings provided herein, including the Figures. It is therefore to be understood that changes can be made in/to the preferred and exemplary embodiments of the present disclosure which are within the scope of the embodiments disclosed herein.

Moreover, it is contemplated that corresponding and/or related systems incorporating and/or implementing the device or such as may be used/implemented in a device in accordance with the present disclosure are also contemplated and considered to be within the scope of the present disclosure. Further, corresponding and/or related method for manufacturing and/or using a device and/or system in accordance with the present disclosure are also contemplated and considered to be within the scope of the present disclosure.

Claims

1. A central signal segregation station (100), comprising:

a signal acquisition controller (103) structurally configured to receive a plurality of different types of physiological signals from a plurality of unknown physiological sensors (10; 20; 30; 40; 50; 60; 70; 80); and

a signal segregation controller (104) in communication with the signal acquisition controller (103),

wherein, responsive to the signal acquisition controller (103) receiving the plurality of different physiological signals, the signal segregation controller (104) is structurally configured to control an identification of a particular type of each physiological signal based on distinct signal features of each physiological signal corresponding to a different physiological signal model (101) among a plurality of physiological signal models (101) derived from known types of physiological sensors.

2. The central signal segregation station (100) of claim 1, wherein the signal segregation controller (104) is further structurally configured to determine a similarity measurement of each physiological signal to each physiological signal model.

3. The central signal segregation station (100) of claim 1, further comprising:

a signal analyzing controller (105) in communication with the signal segregation controller (104),

wherein the signal analyzing controller (105) is structurally configured to control an execution of a signal quality processing of each physiological signal identified by the signal segregation controller (104).

4. The central signal segregation station (100) of claim 3,

wherein the signal analyzing controller (105) is further structurally configured to control a communication of a signal quality of a physiological signal to an associated unknown physiological sensor.

5. The central signal segregation station (100) of claim 1, further comprising:

a signal analyzing controller (105) in communication with the signal segregation controller (104),

wherein the signal analyzing controller (105) is structurally configured to annotate at least one region of each physiological signal identified by the signal segregation controller (104), and

wherein each region of the at least region includes diagnostic information of the corresponding physiological signal.

6. The central signal segregation station (100) of claim 5,

wherein the signal analyzing controller (105) is further structurally configured to control a communication of a personal care plan to an unknown physiological source, and

wherein the person care plan is derived from a diagnosis of the at least one annotated region of the associated physiological signal.

7. The central signal segregation station (100) of claim 6,

wherein the signal analyzing controller (105) is further structurally configured to corroborate the diagnosis of the at least one annotated region of the associated physiological signal based on context aware information appended to the associated physiological signal.

8. A central signal segregation system, comprising:

a plurality of unknown physiological sensors (10; 20; 30; 40; 50; 60; 70; 80) and a central signal segregation station (100);

wherein each unknown physiological sensor (10; 20; 30; 40; 50; 60; 70; 80) is structurally configured to transmit a different type of physiological signal to the central signal segregation station (100); and

wherein, responsive to the central signal segregation station (100) receiving the plurality of different physiological signals, the central signal segregation station (100) is structurally configured to control an identification of a particular type of each physiological signal based on distinct signal features of each physiological signal

corresponding to a different physiological signal model (101) among a plurality of physiological signal models (101) derived from known types of physiological sensors.

9. The central signal segregation system of claim 8, wherein the unknown physiological sensors (10; 20; 30; 40; 50; 60; 70; 80) include at least two of an electrocardiogram monitor, a respiration electrode patch, a pulse oximeter, a blood pressure monitor, a galvanic skin response sensor, a skin temperature sensor, a heat flux sensor and a near body temperature sensor.

10. The central signal segregation system of claim 8, wherein the signal segregation controller (104) is further structurally configured to determine a similarity measurement of each physiological signal to each physiological signal model.

11. The central signal segregation system of claim 8, further comprising:

a signal analyzing controller (105) in communication with the signal segregation controller (104),

wherein the signal analyzing controller (105) is structurally configured to control an execution of a signal quality processing of each physiological signal identified by the signal segregation controller (104).

12. The central signal segregation system of claim 11,

wherein the signal analyzing controller (105) is further structurally configured to control a communication of a signal quality of a physiological signal to an associated unknown physiological sensor.

13. The central signal segregation system of claim 8, further comprising:

a signal analyzing controller (105) in communication with the signal segregation controller (104),

wherein the signal analyzing controller (105) is structurally configured to annotate at least one region of each physiological signal identified by the signal segregation controller (104), and

wherein each region of the at least region includes diagnostic information of the corresponding physiological signal.

14. The central signal segregation system of claim 13,

wherein the signal analyzing controller (105) is further structurally configured to control a communication of a personal care plan to an unknown physiological source, and

wherein the person care plan is derived from a diagnosis of the at least one annotated region of the associated physiological signal.

15. The central signal segregation system of claim 14,

wherein the signal analyzing controller (105) is further structurally configured to corroborate the diagnosis of the at least one annotated region of the associated physiological signal based on context aware information appended to the associated physiological signal.

16. A central signal segregation method, comprising:

a central signal segregation station (100) receiving a plurality of different types of physiological signals from a plurality of unknown physiological sensors (10; 20; 30; 40; 50; 60; 70; 80); and

the central signal segregation station (100) identifying a particular type of each physiological signal based on distinct signal features of each physiological signal corresponding to a different physiological signal model (101) among a plurality of physiological signal models (101) derived from known types of physiological sensors.

17. The central signal segregation method of claim 16, further comprising:

the central signal segregation station (100) executing a signal quality processing of each physiological signal identified by the central signal segregation station (100).

18. The central signal segregation system of claim 8, further comprising:

the central signal segregation station (100) annotating at least one region of each physiological signal identified by the central signal segregation station (100),

wherein each region of the at least region includes diagnostic information of the corresponding physiological signal.

19. The central signal segregation system of claim 18, further comprising:

the central signal segregation station (100) communicating a personal care plan to an unknown physiological source,

wherein the person care plan is derived from a diagnosis of the at least one annotated region of the associated physiological signal.

20. The central signal segregation system of claim 19, further comprising:

the central signal segregation station (100) corroborating the diagnosis of the at least one annotated region of the associated physiological signal based on context aware information appended to the associated physiological signal.

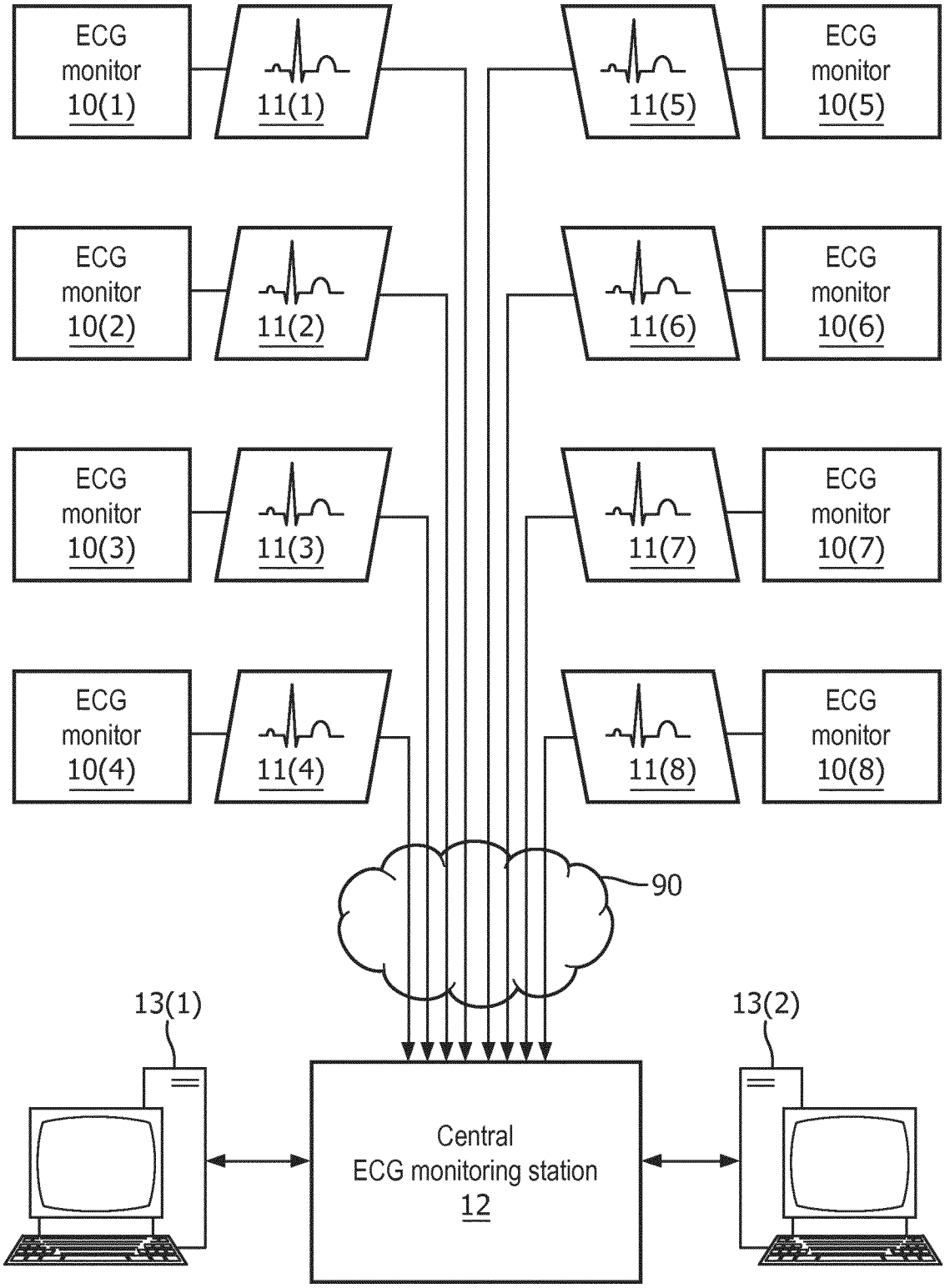

FIG. 1
(prior art)

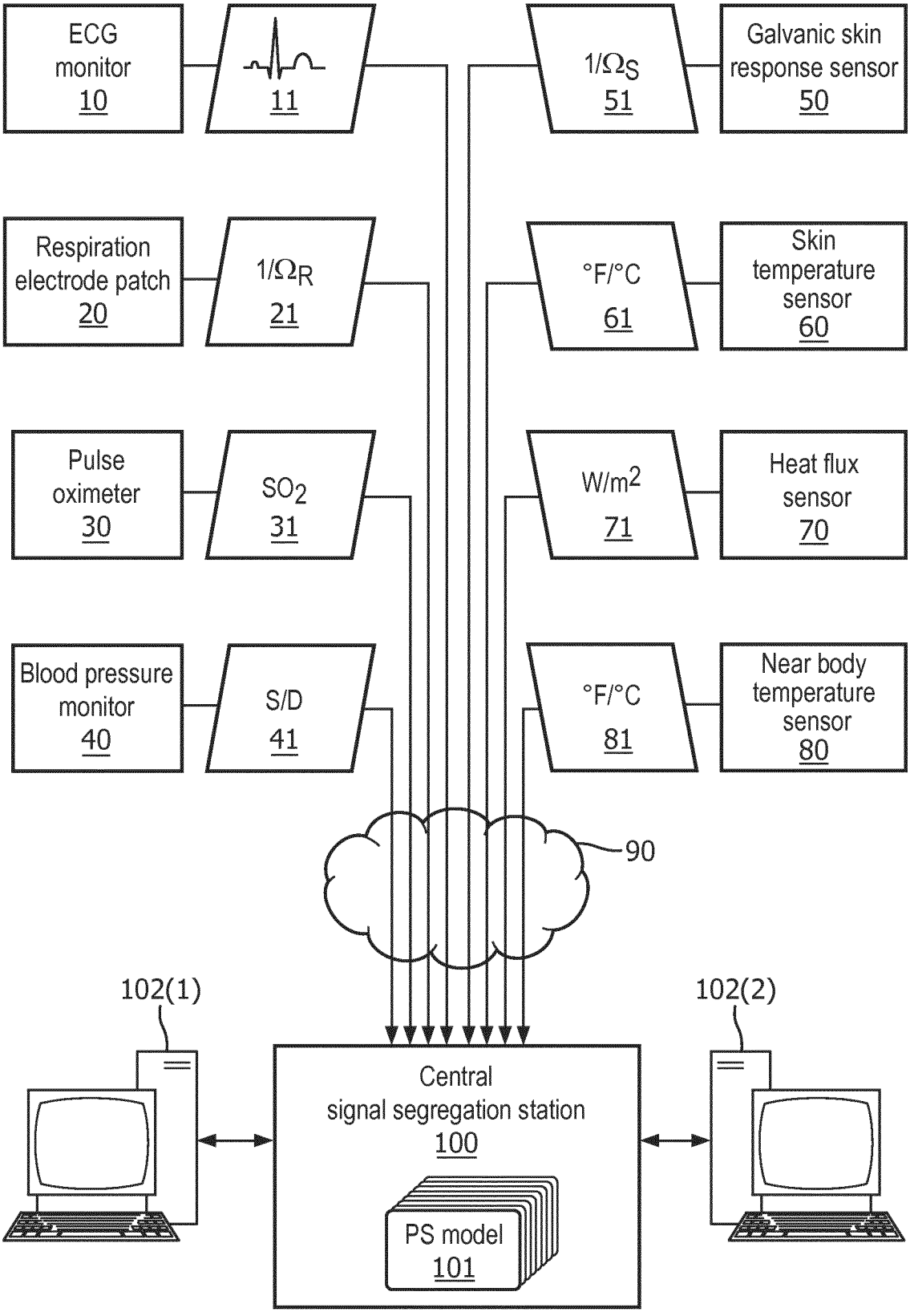
ECG monitor 10
11
1/ΩS 51
Galvanic skin response sensor 50
Respiration electrode patch 20
1/ΩR 21
°F/°C 61
Skin temperature sensor 60
Pulse oximeter 30
SO2 31
W/m2 71
Heat flux sensor 70
Blood pressure monitor 40
S/D 41
°F/°C 81
Near body temperature sensor 80
90
102(1)
102(2)
Central signal segregation station 100
PS model 101

FIG. 2

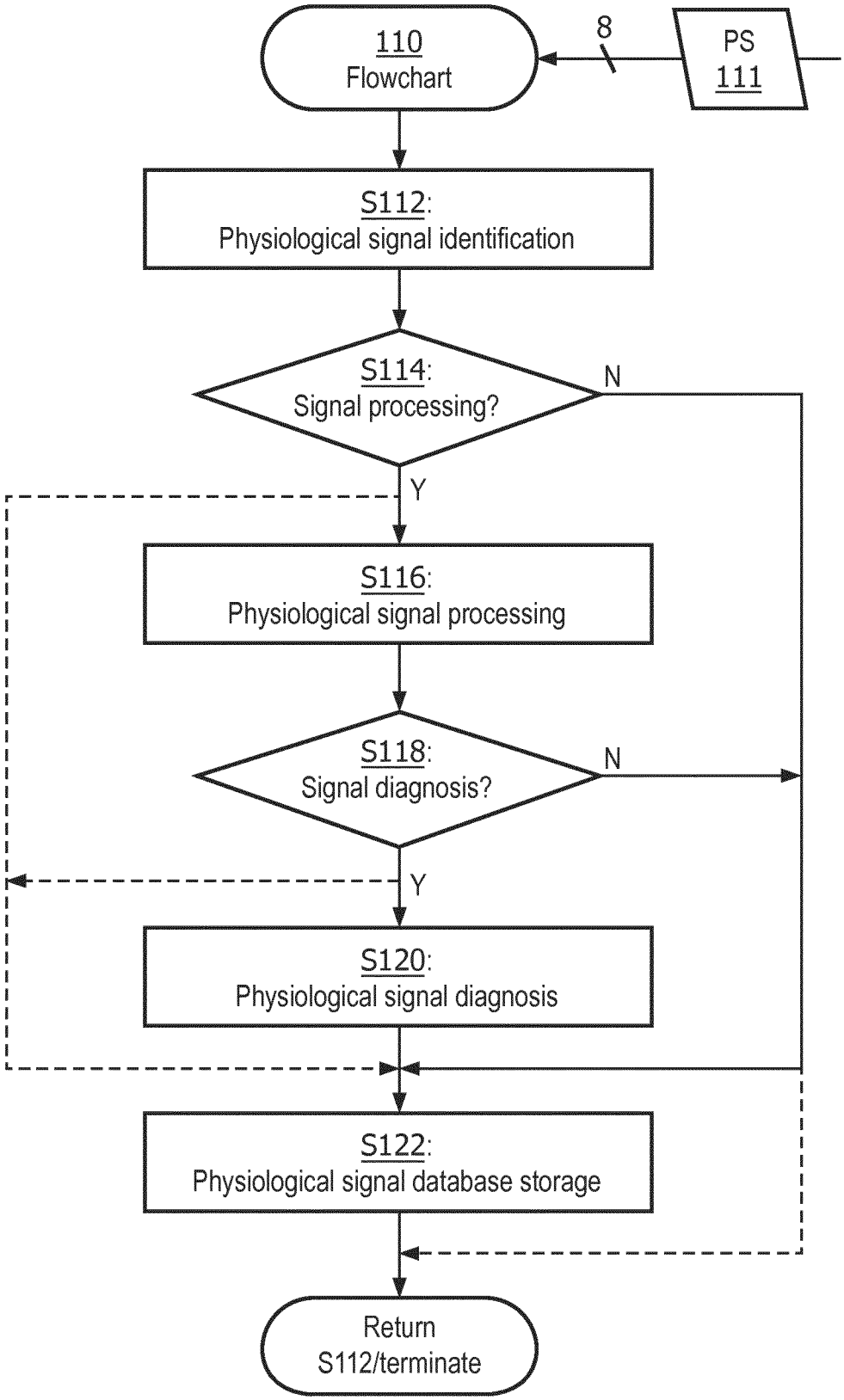
110
Flowchart
8
PS
111
S112:
Physiological signal identification
S114:
Signal processing?
N
Y
S116:
Physiological signal processing
S118:
Signal diagnosis?
N
Y
S120:
Physiological signal diagnosis
S122:
Physiological signal database storage
Return
S112/terminate

FIG. 3

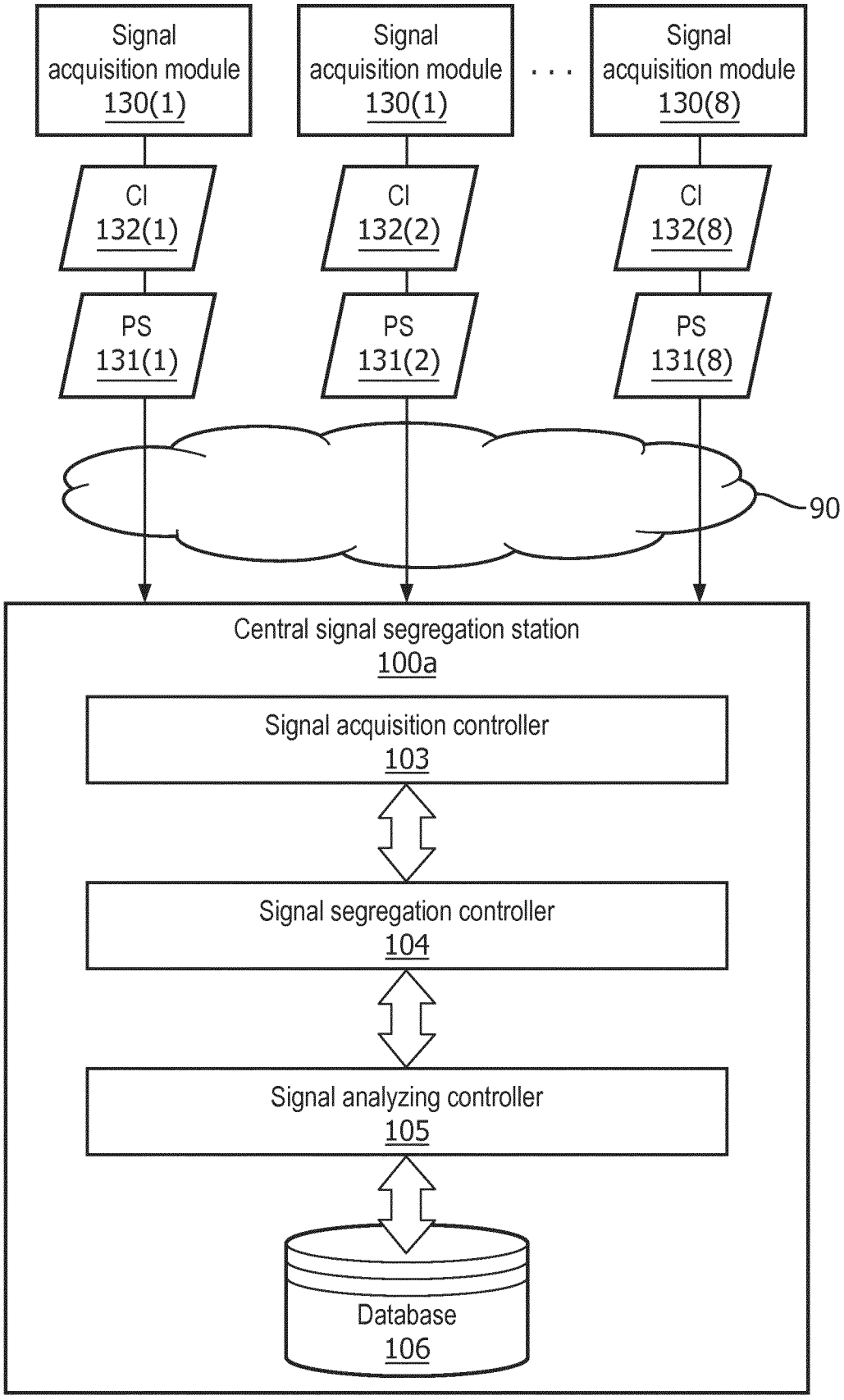
Signal acquisition module 130(1)
Signal acquisition module 130(1)
Signal acquisition module 130(8)
CI 132(1)
CI 132(2)
CI 132(8)
PS 131(1)
PS 131(2)
PS 131(8)
90
Central signal segregation station 100a
Signal acquisition controller 103
Signal segregation controller 104
Signal analyzing controller 105
Database 106

FIG. 4

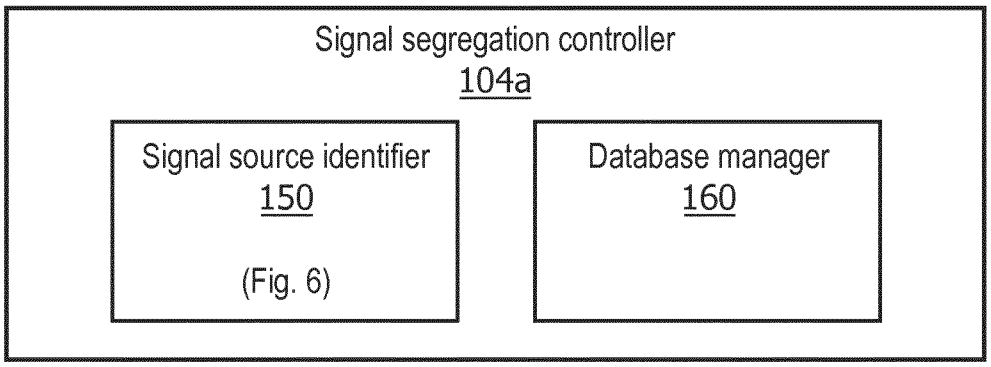
Signal segregation controller
104a
Signal source identifier
150
(Fig. 6)
Database manager
160

FIG. 5A

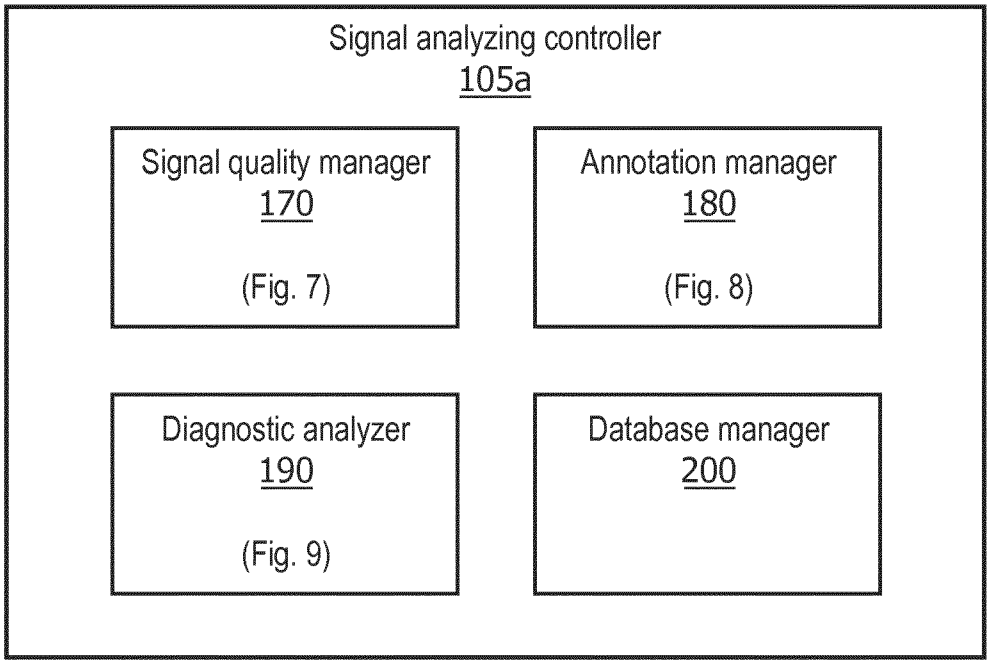
Signal analyzing controller
105a
Signal quality manager
170
(Fig. 7)
Annotation manager
180
(Fig. 8)
Diagnostic analyzer
190
(Fig. 9)
Database manager
200

FIG. 5B

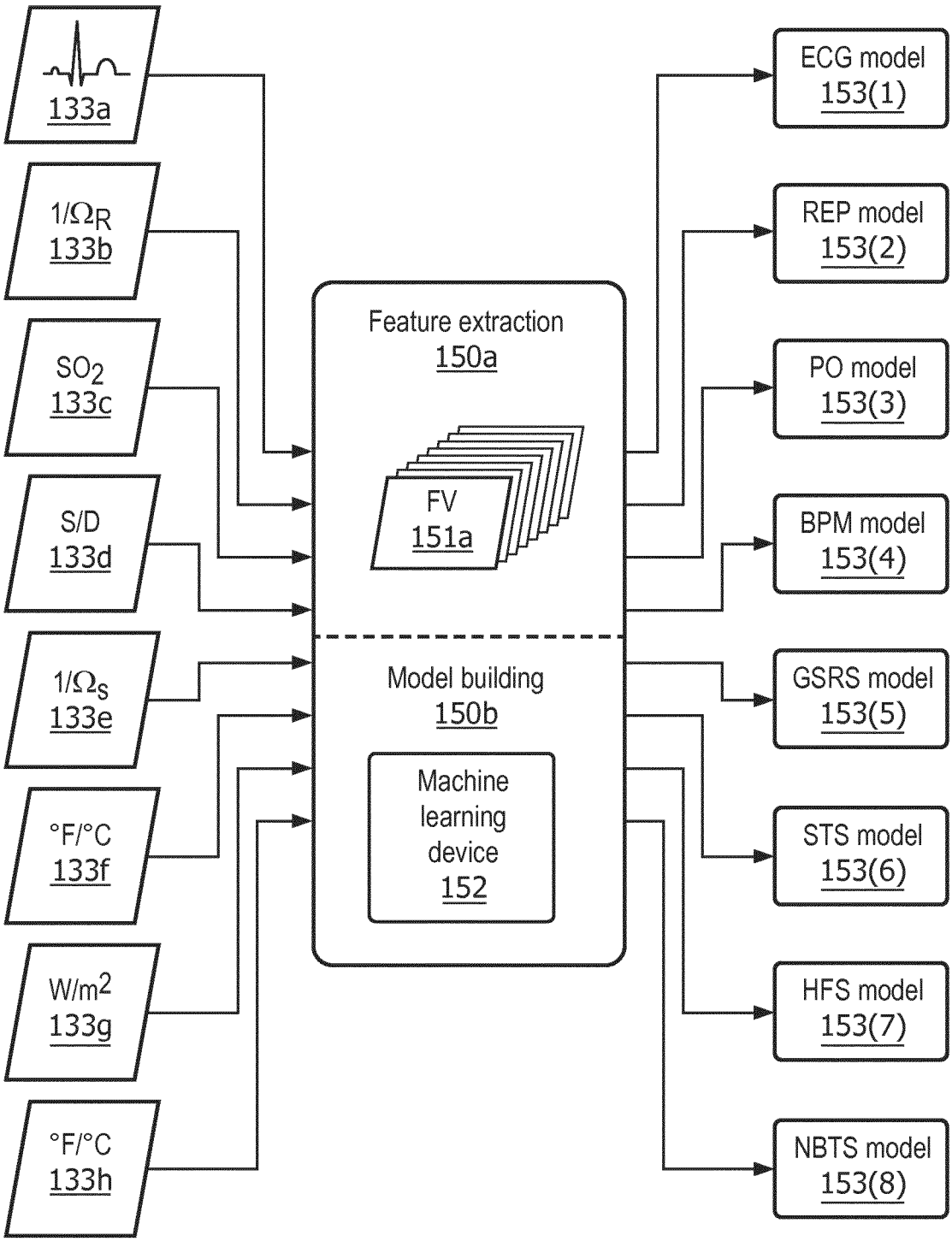
133a
1/ΩR
133b
SO2
133c
S/D
133d
1/Ωs
133e
°F/°C
133f
W/m2
133g
°F/°C
133h
Feature extraction
150a
FV
151a
Model building
150b
Machine learning device
152
ECG model
153(1)
REP model
153(2)
PO model
153(3)
BPM model
153(4)
GSRS model
153(5)
STS model
153(6)
HFS model
153(7)
NBTS model
153(8)

FIG. 6A

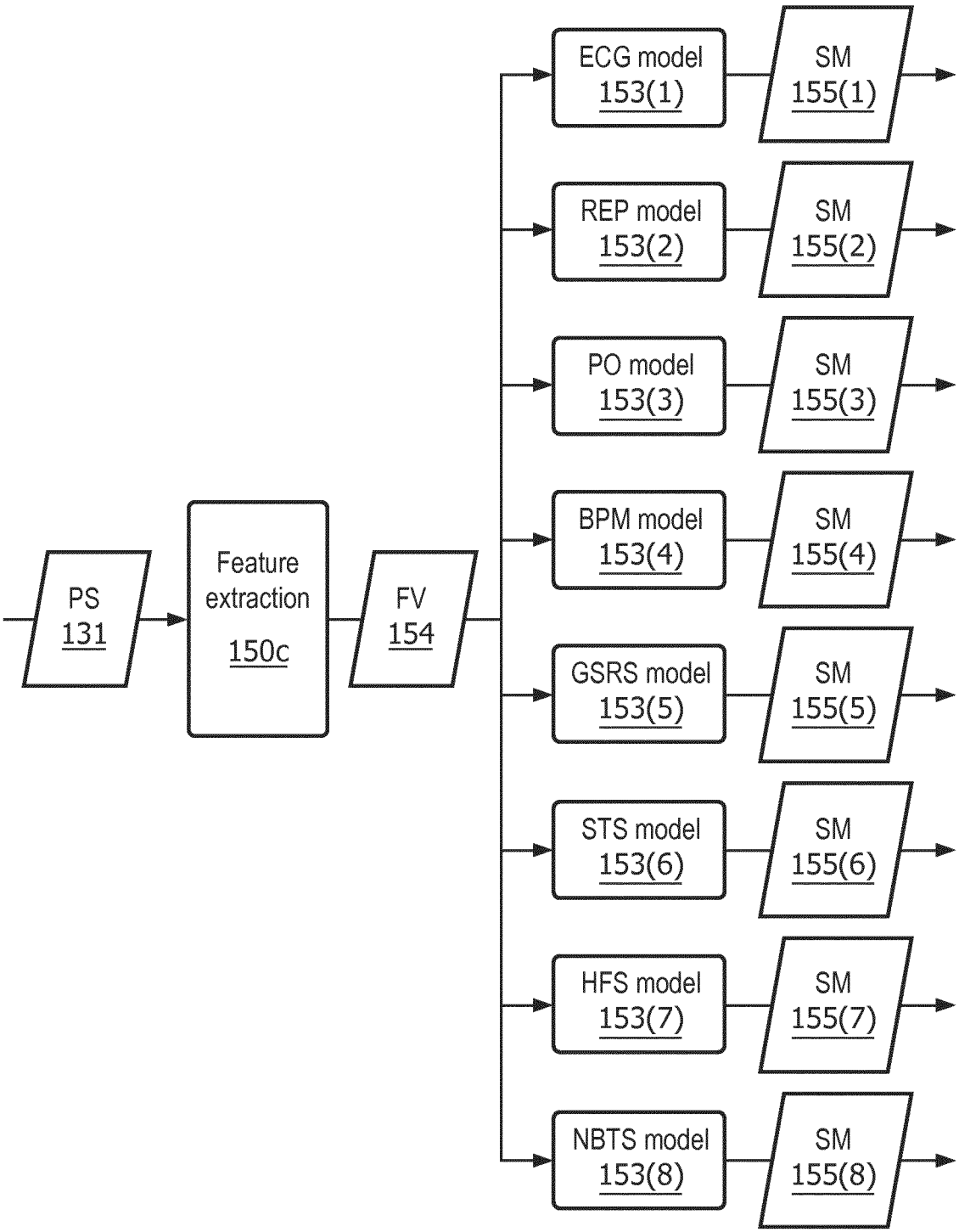
PS
131
Feature extraction
150c
FV
154
ECG model
153(1)
SM
155(1)
REP model
153(2)
SM
155(2)
PO model
153(3)
SM
155(3)
BPM model
153(4)
SM
155(4)
GSRS model
153(5)
SM
155(5)
STS model
153(6)
SM
155(6)
HFS model
153(7)
SM
155(7)
NBTS model
153(8)
SM
155(8)

FIG. 6B

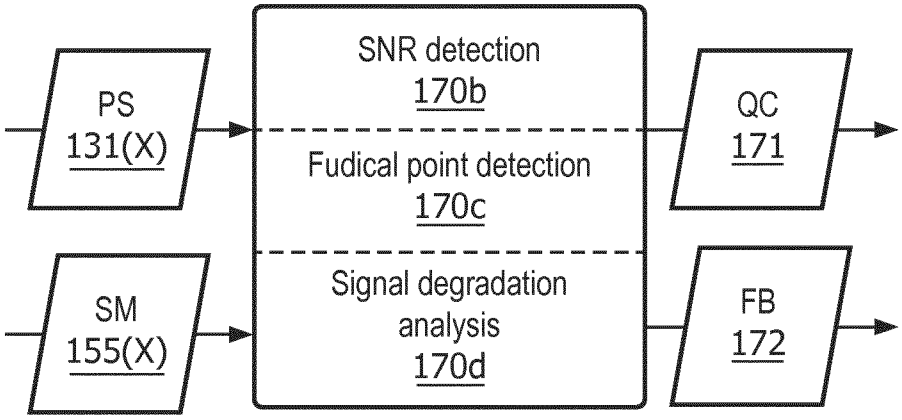

FIG. 7

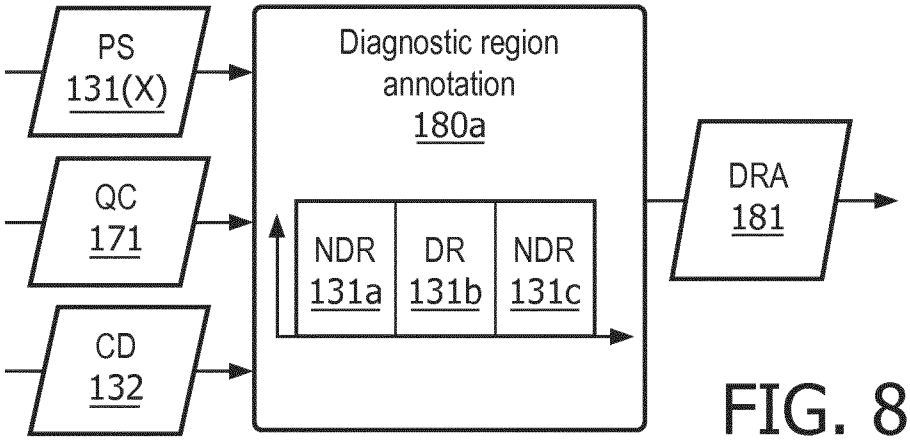

FIG. 8

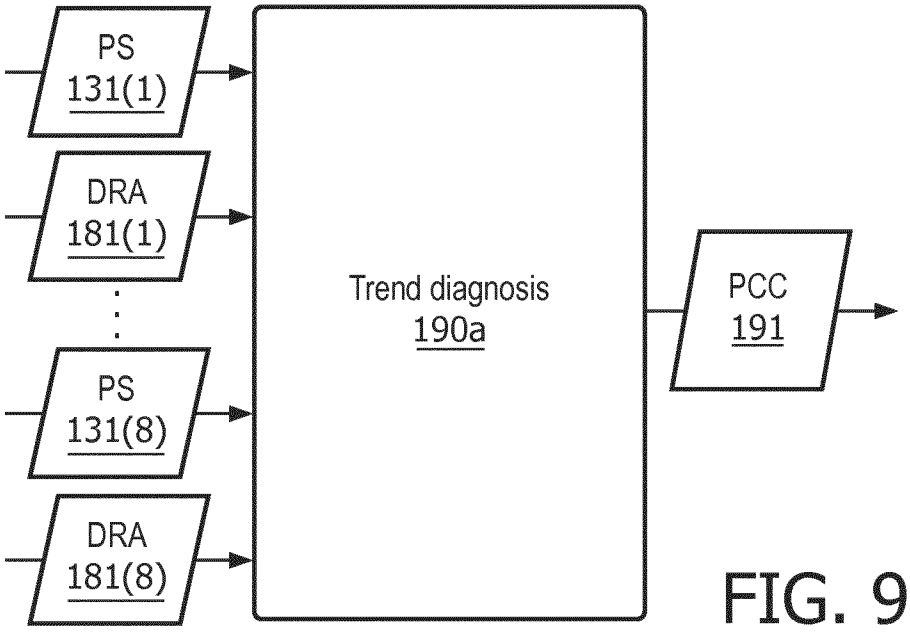

FIG. 9

INTERNATIONAL SEARCH REPORT

International application No
PCT/EP2017/067604

A. CLASSIFICATION OF SUBJECT MATTER
INV. G06F19/00 A61B5/00
ADD.

According to International Patent Classification (IPC) or to both national classification and IPC

B. FIELDS SEARCHED

Minimum documentation searched (classification system followed by classification symbols)
G06F

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

Electronic data base consulted during the international search (name of data base and, where practicable, search terms used)
EPO-Internal, WPI Data

C. DOCUMENTS CONSIDERED TO BE RELEVANT

Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X	US 2005/007091 A1 (MAKEIG SCOTT [US] ET AL) 13 January 2005 (2005-01-13) figures 3,4,5 paragraph [0100] - paragraph [0105] paragraph [0048] - paragraph [0052] paragraph [0124] -----	1-20
A	US 2013/338519 A1 (CHEN YU [US] ET AL) 19 December 2013 (2013-12-19) paragraph [0007] - paragraph [0008] -----	1-20

☐ Further documents are listed in the continuation of Box C.

☒ See patent family annex.

* Special categories of cited documents :

"A" document defining the general state of the art which is not considered to be of particular relevance

"E" earlier application or patent but published on or after the international filing date

"L" document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified)

"O" document referring to an oral disclosure, use, exhibition or other means

"P" document published prior to the international filing date but later than the priority date claimed

"T" later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention

"X" document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone

"Y" document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art

"&" document member of the same patent family

Date of the actual completion of the international search	Date of mailing of the international search report
20 September 2017	28/09/2017

Name and mailing address of the ISA/	Authorized officer
European Patent Office, P.B. 5818 Patentlaan 2 NL - 2280 HV Rijswijk Tel. (+31-70) 340-2040, Fax: (+31-70) 340-3016	Wittke, Claudia

1

INTERNATIONAL SEARCH REPORT

Information on patent family members

International application No
PCT/EP2017/067604

Patent document cited in search report	Publication date	Patent family member(s)	Publication date
US 2005007091 A1	13-01-2005	NONE	
US 2013338519 A1	19-12-2013	CN 103501694 A	08-01-2014
		EP 2688468 A1	29-01-2014
		US 2013338519 A1	19-12-2013
		WO 2012129413 A1	27-09-2012

专利名称(译)	中央信号隔离系统		
公开(公告)号	EP3485406A1	公开(公告)日	2019-05-22
申请号	EP2017739555	申请日	2017-07-12
[标]申请(专利权)人(译)	皇家飞利浦电子股份有限公司		
申请(专利权)人(译)	皇家飞利浦N.V.		
当前申请(专利权)人(译)	皇家飞利浦N.V.		
[标]发明人	PATIL RAVINDRA BALASAHEB PALANISAMY KRISHNAMOORTHY		
发明人	PATIL, RAVINDRA, BALASAHEB PALANISAMY, KRISHNAMOORTHY		
IPC分类号	G06F19/00 A61B5/00		
优先权	62/361853 2016-07-13 US		
外部链接	Espacenet		

摘要(译)

中央信号分离站（100）采用信号采集控制器（103）和信号分离控制器（104）。在操作中，信号采集控制器（103）从多个未知生理传感器（10; 20; 30; 40; 50; 60; 70; 80）接收多种不同类型的生理信号。为了监测生理信号，信号分离控制器（104）基于与多个生理信号模型中的不同生理信号模型（101）相对应的每个生理信号的不同信号特征来识别每种生理信号的特定类型（101）衍生自已知类型的生理传感器。为了分析生理信号，站（100）还可以采用信号分析控制器（105）执行生理信号的信号质量处理，向传送低质量生理信号的任何生理传感器提供信号特定反馈。，注释每个生理信号的特定区域，其具有最大诊断信息和/或执行生理信号的确认诊断。