



(11) **EP 2 938 379 B1**

(12) **EUROPEAN PATENT SPECIFICATION**

(45) Date of publication and mention
of the grant of the patent:

24.04.2019 Bulletin 2019/17

(21) Application number: **13830104.9**

(22) Date of filing: **17.12.2013**

(51) Int Cl.:

A61M 16/00 (2006.01) **A61B 5/00** (2006.01)
A61B 5/08 (2006.01) **A61B 5/087** (2006.01)
A61B 5/091 (2006.01) **A61M 16/10** (2006.01)
A61M 16/16 (2006.01) **A61M 16/20** (2006.01)

(86) International application number:

PCT/IB2013/061012

(87) International publication number:

WO 2014/102659 (03.07.2014 Gazette 2014/27)

(54) **SYSTEM FOR LIMITING FLOW COMPENSATION DURING LIMITED FLOW RESPIRATORY THERAPY**

SYSTEM ZUR BEGRENZUNG VON FLUSSAUSGLEICH BEI EINER ATEMTHERAPIE MIT
BEGRENZTEM FLUSS

SYSTÈME DE LIMITATION D'UNE COMPENSATION D'ÉCOULEMENT PENDANT UNE THÉRAPIE
RESPIRATOIRE À FLUX LIMITÉ

(84) Designated Contracting States:

**AL AT BE BG CH CY CZ DE DK EE ES FI FR GB
GR HR HU IE IS IT LI LT LU LV MC MK MT NL NO
PL PT RO RS SE SI SK SM TR**

(30) Priority: **26.12.2012 US 201261745870 P**

(43) Date of publication of application:

04.11.2015 Bulletin 2015/45

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Description

[0001] The present disclosure pertains to a pressure support system configured to deliver a pressurized flow of breathable gas to the airway of a subject. The pressure support system is configured to determine a compensation limit for a compensation amount of a gas parameter based on a current leak value.

[0002] Systems to treat obstructive sleep apnea (OSA) are known. Typically, OSA is treated via positive airway pressure (PAP). There are multiple methods available to deliver PAP. The most common method is continuous positive airway pressure (CPAP). Traditional therapies may be uncomfortable for some patients. Breathing in while air is being forced into the airway using positive airway pressure may feel uncomfortable and/or unnatural to some patients.

[0003] WO 2008/100859 discloses a pressure support system and method with automatic comfort feature modification.

[0004] US 2006/0000475 discloses a bi-level pressure support system and method of treating disordered breathing that optimizes the pressure delivered to the patient during inspiration/expirations to treat the disordered breathing while minimizing the delivered pressure for patient comfort.

[0005] WO 2005/051469 discloses a method and apparatus for providing ventilatory assistance to a spontaneously breathing patient.

[0006] WO 2009/112076 discloses a respirator having a variable pressure support.

[0007] US 2008/0295837 discloses a method to limit leak compensation of a delivered tidal volume based on a breathing circuit leak alarm. According to the teaching of this document, when an average leak volume exceeds an alarm threshold, such as a set volume or a set percentage of tidal volume, the tidal volume delivered by the ventilator is limited to be equal to the current tidal volume being delivered when the leak alarm was first generated.

[0008] According to the invention, a pressure support system according to claim 1 is provided. Said pressure support system is configured to deliver a pressurized flow of breathable gas to the airway of a subject. The pressure support system comprises a pressure generator, one or more sensors, and one or more processors. The pressure generator is configured to generate the pressurized flow of breathable gas. The one or more sensors are configured to generate output signals conveying information related to one or more gas parameters of the pressurized flow of breathable gas. The one or more processors are configured to execute computer program modules. The computer program modules comprise a leak module, a control module, a compensation module, and a compensation limit module. The leak module is configured to estimate a current leak value. The control module is configured to control operation of the pressure generator to generate the pressurized flow of breathable gas according to a limited flow mode therapy regime that dictates a therapeutic level of a flow rate of the one or more gas parameters at or near the airway of the subject. The compensation module is configured to determine a compensation amount to adjust the flow rate to compensate for respiratory effort during inhalation to maintain the therapeutic level for the flow rate. The compensation module is configured to determine the compensation amount based on the therapeutic level and the output signals. The control module is configured to control the pressure generator to generate the pressurized flow of breathable gas with the flow rate at a level that reflects the compensation amount. The compensation limit module is configured to determine a compensation limit for the compensation amount of the flow rate based on the current leak value. The compensation module is configured to implement the compensation limit as a limit for the compensation amount. The current leak value is an instantaneous indication of the amount of leak in the pressure support system. The compensation limit module is configured to determine a flow rate compensation limit that is one to two times the current leak value.

[0009] According to a comparative example not falling within the scope of the invention, a method for providing a pressurized flow of breathable gas with a pressure support system may be provided. The pressure support system comprises a pressure generator for generating the pressurized flow of breathable gas, one or more sensors, and one or more processors. The one or more processors are configured to execute computer program modules. The computer program modules comprise a leak module, a control module, a compensation module, and a compensation limit module. The method comprises generating output signals conveying information related to one or more gas parameters of the pressurized flow of breathable gas with the one or more sensors; estimating a current leak value with the leak module; controlling, with the control module, operation of the pressure generator to generate the pressurized flow of breathable gas according to a limited flow mode therapy regime that dictates a therapeutic level of a first gas parameter of the one or more gas parameters at or near the airway of a subject; determining a compensation amount, with the compensation module, to adjust the first gas parameter to compensate for respiratory effort during inhalation to maintain the therapeutic level for the first gas parameter, wherein determining the compensation amount is based on the therapeutic level and the output signals; controlling, with the control module, generation of the pressurized flow of breathable gas with the first gas parameter at a level that reflects the compensation amount; determining a compensation limit, with the compensation limit module, for the compensation amount of the first gas parameter based on the current leak value; and implementing, with the compensation module, the compensation limit as a limit for the compensation amount.

[0010] According to a comparative example not falling within the scope of the invention, a pressure support system may be provided. The system is configured to deliver a pressurized flow of breathable gas to the airway of a subject. The pressure support system comprises means for generating the pressurized flow of breathable gas; means for gen-

erating output signals conveying information related to one or more gas parameters of the pressurized flow of breathable gas; and means for executing computer program modules. The computer program modules comprise means for estimating a current leak value; means for controlling operation of the means for generating the pressurized flow of breathable gas to generate the pressurized flow of breathable gas according to a limited flow mode therapy regime that dictates a therapeutic level of a first gas parameter of the one or more gas parameters at or near the airway of the subject; means for determining a compensation amount to adjust the first gas parameter to compensate for respiratory effort during inhalation to maintain the therapeutic level for the first gas parameter, wherein the means for determining a compensation amount is configured to determine the compensation amount based on the therapeutic level and the output signals, wherein the means for controlling operation is configured to control the means for generating the pressurized flow of breathable gas to generate the pressurized flow of breathable gas with the first gas parameter at a level that reflects the compensation amount; and means for determining a compensation limit for the compensation amount of the first gas parameter based on the current leak value, wherein the means for determining a compensation is configured to implement the compensation limit as a limit for the compensation amount.

[0011] These and other features and characteristics of the present disclosure, as well as the methods of operation and functions of the related elements of structure and the combination of parts and economies of manufacture, will become more apparent upon consideration of the following description and the appended claims with reference to the accompanying drawings, all of which form a part of this specification, wherein like reference numerals designate corresponding parts in the various figures. It is to be expressly understood, however, that the drawings are for the purpose of illustration and description only and are not intended as a definition of the limits of the invention, which is solely defined by the scope of claim 1.

FIG. 1 is a schematic illustration of a pressure support system configured to deliver a pressurized flow of breathable gas to the airway of a subject, according to an embodiment of the invention.

FIG. 2 illustrates a method for delivering a pressurized flow of breathable gas to the airway of a subject with a pressure support system, according to a comparative example not falling within the scope of the invention.

[0012] As used herein, the singular form of "a", "an", and "the" include plural references unless the context clearly dictates otherwise. As used herein, the statement that two or more parts or components are "coupled" shall mean that the parts are joined or operate together either directly or indirectly, i.e., through one or more intermediate parts or components, so long as a link occurs. As used herein, "directly coupled" means that two elements are directly in contact with each other. As used herein, "fixedly coupled" or "fixed" means that two components are coupled so as to move as one while maintaining a constant orientation relative to each other.

[0013] As used herein, the word "unitary" means a component is created as a single piece or unit. That is, a component that includes pieces that are created separately and then coupled together as a unit is not a "unitary" component or body. As employed herein, the statement that two or more parts or components "engage" one another shall mean that the parts exert a force against one another either directly or through one or more intermediate parts or components. As employed herein, the term "number" shall mean one or an integer greater than one (i.e., a plurality).

[0014] Directional phrases used herein, such as, for example and without limitation, top, bottom, left, right, upper, lower, front, back, and derivatives thereof, relate to the orientation of the elements shown in the drawings and are not limiting upon the claims unless expressly recited therein.

[0015] FIG. 1 is a schematic illustration of a pressure support system 10 configured to deliver a pressurized flow of breathable gas to the airway of a subject 12. System 10 is configured to treat obstructive sleep apnea, other sleep disordered breathing, and/or other respiratory issues with limited flow respiration therapy, and/or other therapies. Limited flow respiration therapy may be an alternative to CPAP, for example. Limited flow respiration therapy is described in described in United States Patent Application No. Philips Ref # 2011P00603US - ID774330 filed July 01, 2011, entitled "System and Method for Limited Flow Respiration Therapy". System 10 is configured to limit flow rate compensation during inspiration to values proportional to the current leak to achieve limited flow respiration therapy. System 10 comprises one or more of a pressure generator 14, a subject interface 16, one or more sensors 18, a processor 20, a user interface 22, electronic storage 24, and optionally other components.

[0016] Pressure generator 14 is configured to generate a pressurized flow of breathable gas for delivery to the airway of subject 12. Pressure generator 14 controls the flow rate of the flow of gas for therapeutic purposes. Pressure generator 14 is configured to control the flow rate of the flow of gas to provide limited flow respiration therapy to the airway of subject 12.

[0017] Pressure generator 14 receives a flow of gas from a gas source, such as the ambient atmosphere, and elevates and/or reduces the pressure of that gas for delivery to the airway of a patient. Pressure generator 14 is any device, such as, for example, a pump, blower, piston, or bellows, that is capable of elevating and/or reducing the pressure of the received gas for delivery to a patient. Pressure generator 14 may comprise one or more valves for controlling the pressure and/or flow of gas, for example. The present disclosure also contemplates controlling the operating speed of the blower,

either alone or in combination with such valves, to control the flow of gas provided to the patient.

[0018] Subject interface 16 is configured to deliver the pressurized flow of breathable gas to the airway of subject 12. As such, subject interface 16 comprises conduit 30, interface appliance 32, and/or other components. Conduit 30 is configured to convey the pressurized flow of gas to interface appliance 32. Conduit 30 may be a flexible length of hose, or other conduit, that places interface appliance 32 in fluid communication with pressure generator 14. Interface appliance 32 is configured to deliver the flow of gas to the airway of subject 12. In some embodiments, interface appliance 32 is non-invasive. As such, interface appliance 32 non-invasively engages subject 12. Non-invasive engagement comprises removably engaging an area (or areas) surrounding one or more external orifices of the airway of subject 12 (e.g., nostrils and/or mouth) to communicate gas between the airway of subject 12 and interface appliance 32. Some examples of non-invasive interface appliance 32 may comprise, for example, a nasal cannula, a nasal mask, a nasal/oral mask, a full face mask, a total face mask, or other interface appliances that communicate a flow of gas with an airway of a subject. The present disclosure is not limited to these examples, and contemplates delivery of the flow of gas to the subject using any interface appliance, including an invasive interface appliance such as an endotracheal tube and/or other appliances.

[0019] Sensors 18 are configured to generate output signals conveying information related to one or more gas parameters of the pressurized flow of breathable gas. The one or more gas parameters may comprise one or more of a flow rate, a volume, a pressure, a composition (e.g., concentration(s) of one or more constituents), temperature, humidity, acceleration, velocity, acoustics, changes in a parameter indicative of respiratory effort by subject 12, and/or other gas parameters. Sensors 18 may comprise one or more sensors that measure such parameters directly (e.g., through fluid communication with the flow of gas in subject interface 16). Sensors 18 may comprise one or more sensors that generate output signals related to one or more parameters of the flow of gas indirectly. For example, one or more of sensors 18 may generate an output based on an operating parameter of pressure generator 14 (e.g., a valve driver or motor current, voltage, rotational velocity, and/or other operating parameters). Although sensors 18 are illustrated at a single location within (or in communication with) conduit 30 between interface appliance 32 and pressure generator 14, this is not intended to be limiting. Sensors 18 may include sensors disposed in a plurality of locations, such as for example, within pressure generator 14, within (or in communication with) interface appliance 32, in communication with subject 12, and/or in other locations.

[0020] Processor 20 is configured to provide information processing capabilities in system 10. As such, processor 20 may comprise one or more of a digital processor, an analog processor, a digital circuit designed to process information, an analog circuit designed to process information, a state machine, and/or other mechanisms for electronically processing information. Although processor 20 is shown in FIG. 1 as a single entity, this is for illustrative purposes only. In some implementations, processor 20 may comprise a plurality of processing units. These processing units may be physically located within the same device (e.g., pressure generator 14), or processor 20 may represent processing functionality of a plurality of devices operating in coordination.

[0021] As shown in FIG. 1, processor 20 is configured to execute one or more computer program modules. The one or more computer program modules comprise a parameter module 50, a leak module 52, a control module 54, a compensation module 56, a compensation limit module 58, and optionally other modules. Processor 20 may be configured to execute modules 50, 52, 54, 56, and/or 58 by software; hardware; firmware; some combination of software, hardware, and/or firmware; and/or other mechanisms for configuring processing capabilities on processor 20.

[0022] It should be appreciated that although modules 50, 52, 54, 56, and 58 are illustrated in FIG. 1 as being co-located within a single processing unit, in implementations in which processor 20 comprises multiple processing units, one or more of modules 50, 52, 54, 56, and/or 58 may be located remotely from the other modules. As another example, processor 20 may be configured to execute one or more additional modules that may perform some or all of the functionality attributed below to one of modules 50, 52, 54, 56, and/or 58.

[0023] Parameter module 50 is configured to determine one or more parameters within system 10. The one or more parameters within system 10 may comprise gas parameters related to the pressurized flow of breathable gas, and/or other parameters. Parameter module 50 is configured to determine the one or more parameters based on the output signals of sensors 18. The information determined by parameter module 50 may be used for controlling pressure generator 14, stored in electronic storage 24, and/or used for other uses. The one or more gas parameters of the pressurized flow of breathable gas may comprise, for example, one or more of a flow rate, a volume, a pressure, humidity, temperature, acceleration, velocity, and/or other gas parameters.

[0024] In some embodiments, parameter module 50 may be configured to determine the respiratory phase (e.g., inhalation, exhalation) during breathing of subject 12. The respiratory phase determinations made by parameter module 50 are based on the output signals from sensors 18, parameter information determined by parameter module 50, and/or other information. Parameter module 50 may be configured to determine additional breathing parameters related to the respiration of subject 12. Additional breathing parameters related to the respiration of subject 12 may comprise a tidal volume, a timing (e.g., beginning and/or end of inhalation, beginning and/or end of exhalation, etc.), a respiration rate, a duration (e.g., of inhalation, of exhalation, of a single breathing cycle, etc.), respiration frequency, and/or other breathing parameters. The respiratory phase determinations may be used by control module 54 to control pressure generator 14

to control the pressurized flow of breathable gas delivered to subject 12, may be stored in electronic storage 24, and/or used for other uses. In some embodiments, parameter module 50 is configured to determine the respiratory phase (e.g., inhalation, exhalation) based on changes in pressure, flow rate, and/or other parameters determined by parameter module 50.

[0025] Leak module 52 is configured to estimate a current leak value. The current leak value is an instantaneous indication of the amount of leak in system 10. The current leak value may be estimated based on one or more of the gas parameters determined by parameter module 50, a therapeutic level of a gas parameter, known properties of subject interface 16 (e.g., of conduit 30 and/or interface appliance 32), and/or other parameters, properties, or variables. The current leak value may be estimated based on a total flow rate, for example. The total flow rate may include a therapeutic flow rate delivered to subject 12 during inhalation and/or exhalation, and leak. The estimated current leak value may include intentional leak (e.g., to prevent rebreathing) and/or unintentional leak (e.g., mask or mouth leak).

[0026] Control module 54 is configured to control operation of pressure generator 14 to generate the pressurized flow of breathable gas according to a limited flow mode respiratory therapy regime. The limited flow mode respiratory therapy regime dictates therapeutic levels of a first gas parameter of the one or more gas parameters, the first gas parameter being a flow rate at or near the airway of the subject. In some embodiments, the limited flow mode respiratory therapy regime may dictate therapeutic levels of parameters in addition to the first gas parameter. Control module 54 is configured to control pressure generator 14 based on information related to the output signals from sensors 18, information determined by parameter module 50, information entered by a user to user interface 22, and/or other information. The pressurized flow of breathable gas generated by the pressure generator is controlled to replace and/or complement a patient's regular breathing.

[0027] In some comparative examples not falling within the scope of the invention, control module 54 is configured such that the first gas parameter is a pressure. According to the invention, control module 54 is configured such that the first gas parameter is a flow rate. In some comparative examples not falling within the scope of the invention, control module 54 is configured such that the first gas parameter is a parameter other than a pressure and/or a flow rate. Control module 54 may be configured to receive information associated with control inputs related to whether the first gas parameter is a flow rate, a pressure, and/or other parameters entered and/or selected by a user (e.g., subject 12) via user interface 22, and/or other devices. Control module 54 may be configured such that the received information indicates whether the first gas parameter is a flow rate, a pressure, and/or other parameters.

[0028] In some embodiments of the invention, control module 54 may be configured to control pressure generator 14 to generate the flow of gas in accordance with a ventilation and/or positive airway pressure support therapy regime in addition to the limited flow mode respiratory therapy regime. By way of non-limiting example, control module 54 may control pressure generator 14 such that the pressure support provided to the subject via the flow of gas comprises continuous positive airway pressure support (CPAP), bi-level positive airway pressure support (BPAP), proportional positive airway pressure support (PPAP), and/or other types of pressure support therapy, in addition to the limited flow mode respiratory therapy regime.

[0029] Compensation module 56 is configured to determine a compensation amount to adjust the first gas parameter to compensate for respiratory effort during inhalation. Compensation module 56 is configured to determine the compensation amount such that the therapeutic levels for the first gas parameter are maintained. Control module 54 is configured to control pressure generator 14 to generate the pressurized flow of breathable gas with the first gas parameter at a level that reflects the compensation amount.

[0030] Compensation module 56 is configured to determine the compensation amount based on the therapeutic levels and the output signals. In a comparative example not falling within the scope of the invention, the limited flow mode respiratory therapy regime may dictate therapeutic levels for a pressure. The output signals from sensors 18 may convey information related to an actual pressure. The actual pressure may be determined by parameter module 50. The actual pressure may vary with respiratory effort exerted by subject 12. Compensation module 56 may determine a compensation amount to adjust the pressure that corresponds to differences between the actual pressure and the therapeutic pressure. In some embodiments, compensation module 56 may be configured such that lower compensation amounts are determined for actual pressures that are closer to therapeutic levels, and higher compensation amounts are determined for actual pressures that are farther from therapeutic levels.

[0031] Compensation module 56 is configured to determine one or more compensation amounts during an inhalation, and optionally during an exhalation. In some examples, the compensation amount determinations may be continuous during the limited flow respiratory therapy. The number and/or nature (e.g., continuous) of compensation amounts determined by compensation module 56 may be configurable by a user (e.g., a doctor, a caregiver, subject 12) via user interface 22, and/or other components of system 10. Control module 54 is configured to control pressure generator 14 to generate the pressurized flow of breathable gas with the first gas parameter at levels that reflect the compensation amounts.

[0032] Compensation limit module 58 is configured to determine a compensation limit for the compensation amount of the first gas parameter. Compensation limit module 58 is configured to determine the compensation limit based on

the current leak value. Compensation module 56 is configured to implement the compensation limit as a limit for the compensation amount. In some examples, compensation limit module 58 may be configured to determine a compensation limit based on the current leak value via an algorithm. The current leak value is an input into the algorithm. The algorithm may be determined at manufacture, set and/or adjust by a user via user interface 22, and/or determined by other methods.

In some comparative examples not falling within the scope of the invention, compensation limit module 58 may be configured to determine the compensation limit based on previous respiration by subject 12. In some comparative examples not falling within the scope of the invention, the compensation limit may be entered and/or selected by a user via user interface 22. In some implementations, compensation limit module 58 may be configured to titrate the compensation limit based on preferences of subject 12 (e.g., to increase comfort during therapy).

[0033] As described above, the first gas parameter is, according to the invention, a flow rate, and, according to comparative examples not falling within the scope of the invention, may comprise a pressure and/or other gas parameters. Determining a compensation limit for the compensation amount of the flow rate or the pressure based on the current leak value (compensation limit module 58), and implementing the flow rate or the pressure compensation limit as a limit for the compensation amount (compensation module 56), achieves limited flow respiratory therapy that ensures that an effective therapeutic pressure is maintained, but during inspiration (e.g., when the flow rate is greater than leak), that additional flow (above therapeutic levels) is not compensated for. This achieves the desired limited flow respiratory therapy while providing a smooth and comfortable flow rate and pressure profile to subject 12.

[0034] According to the invention, compensation limit module 58 is configured to determine a flow rate compensation limit. According to the invention, compensation limit module 58 is configured to determine a flow rate compensation limit that is one to two times the current leak value. Compensation limit module 58 is configured to determine the flow rate compensation limit as shown below:

$$\text{Flow Rate Compensation}_{\text{limit}} = [X] \times \text{current leak}$$

where $[X] = \{X \in \text{any real number} \mid 1 \leq X \leq 2\}$

[0035] By way of a non-limiting example, during inspiration, responsive to compensation module 56 implementing the flow rate compensation limit, as the compensated flow rate reaches the flow rate compensation limit, control module 54 may control pressure generator 14 to reduce a subject interface 16 mask (for example) pressure. During expiration, the flow rate may be lower than and/or approximately equal to the leak value, such that system 10 may provide therapeutic pressure compensation.

[0036] In some comparative examples not falling within the scope of the invention, compensation limit module 58 is configured to determine a pressure compensation limit. In some comparative examples not falling within the scope of the invention, compensation limit module 58 is configured to determine a pressure compensation limit that is a function of one to two times the current leak value. Compensation limit module 58 is configured to determine the pressure compensation limit as shown below:

$$\text{Pressure Compensation}_{\text{limit}} \approx f([X] \times \text{current leak})$$

where $[X] = \{X \in \text{any real number} \mid 1 \leq X \leq 2\}$

[0037] In this comparative example not falling within the scope of the invention, the pressure compensation is limited to a maximum of the pressure compensation limit value. The pressure compensation limited examples differ from the invention, wherein the flow rate compensation is limited, because, in the pressure compensation limited examples, the flow rate limiting occurs indirectly as a result of limiting the compensated pressure. In the flow rate compensation limited invention, the flow rate compensation is limited directly, before the pressure compensation limit determination.

[0038] User interface 22 is configured to receive entry and/or selection of control inputs from subject 12 and/or other users that select whether system 10 operates in the flow compensation limit mode according to the invention, or the pressure compensation limit mode according to a comparative example not falling within the scope of the invention. Other users may comprise a caregiver, a doctor, a decision maker, and/or other users. This enables data, cues, results, and/or instructions and any other communicable items, collectively referred to as "information," to be communicated between a user (e.g., subject 12) and one or more of pressure generator 14, processor 20, and/or other components of system 10. Examples of interface devices suitable for inclusion in user interface 22 comprise a keypad, buttons, switches, a keyboard, knobs, levers, a display screen, a touch screen, speakers, a microphone, an indicator light, an audible alarm, a printer, a tactile feedback device, and/or other interface devices. In some embodiments, user interface 22 comprises a plurality of separate interfaces. In some embodiments, user interface 22 comprises at least one interface that is provided integrally with pressure generator 14.

[0039] It is to be understood that other communication techniques, either hardwired or wireless, are also contemplated by the present disclosure as user interface 22. For example, the present disclosure contemplates that user interface 22 may be integrated with a removable storage interface provided by electronic storage 24. In this example, information may be loaded into system 10 from removable storage (e.g., a smart card, a flash drive, a removable disk, etc.) that enables the user(s) to customize the implementation of system 10. Other exemplary input devices and techniques adapted for use with system 10 as user interface 22 comprise, but are not limited to, an RS-232 port, RF link, an IR link, modem (telephone, cable or other). In short, any technique for communicating information with system 10 is contemplated by the present disclosure as user interface 22.

[0040] In some embodiments, electronic storage 24 comprises electronic storage media that electronically stores information. The electronic storage media of electronic storage 24 may comprise one or both of system storage that is provided integrally (i.e., substantially non-removable) with system 10 and/or removable storage that is removably connectable to system 10 via, for example, a port (e.g., a USB port, a firewire port, etc.) or a drive (e.g., a disk drive, etc.). Electronic storage 24 may comprise one or more of optically readable storage media (e.g., optical disks, etc.), magnetically readable storage media (e.g., magnetic tape, magnetic hard drive, floppy drive, etc.), electrical charge-based storage media (e.g., EPROM, RAM, etc.), solid-state storage media (e.g., flash drive, etc.), and/or other electronically readable storage media. Electronic storage 24 may store software algorithms, information determined by processor 20, information received via user interface 22, and/or other information that enables system 10 to function properly. Electronic storage 24 may be (in whole or in part) a separate component within system 10, or electronic storage 24 may be provided (in whole or in part) integrally with one or more other components of system 10 (e.g., user interface 22, processor 20, etc.).

[0041] FIG. 2 illustrates a method 200, according to a comparative example not falling within the scope of the invention, for delivering a pressurized flow of breathable gas to the airway of a subject with a pressure support system. The pressure support system comprises a pressure generator, one or more sensors, and/or one or more processors. The one or more processors are configured to execute computer program modules. The computer program modules comprise a leak module, a control module, a compensation module, and a compensation limit module. The operations of method 200 presented below are intended to be illustrative. In some examples, method 200 may be accomplished with one or more additional operations not described, and/or without one or more of the operations discussed. Additionally, the order in which the operations of method 200 are illustrated in FIG. 2 and described below is not intended to be limiting.

[0042] In some examples, method 200 may be implemented in one or more processing devices (e.g., a digital processor, an analog processor, a digital circuit designed to process information, an analog circuit designed to process information, a state machine, and/or other mechanisms for electronically processing information). The one or more processing devices may include one or more devices executing some or all of the operations of method 200 in response to instructions stored electronically on an electronic storage medium. The one or more processing devices may include one or more devices configured through hardware, firmware, and/or software to be specifically designed for execution of one or more of the operations of method 200.

[0043] At an operation 202, the pressurized flow of breathable gas is generated. In some examples, operation 202 is performed by a pressure generator the same as or similar to pressure generator 14 (shown in FIG. 1 and described herein).

[0044] At an operation 204, output signals conveying information related to one or more gas parameters of the pressurized flow of breathable gas are generated. In some examples, operation 204 is performed by sensors the same as or similar to sensors 18 (shown in FIG. 1 and described herein).

[0045] At an operation 206, a current leak value may be estimated. In some examples, operation 206 is performed by a computer program module the same as or similar to leak module 52 (shown in FIG. 1 and described herein).

[0046] At an operation 208, the pressure generator may be controlled according to a limited flow therapy regime. Operation of the pressure generator may be controlled to generate the pressurized flow of breathable gas according to the limited flow mode therapy regime. The limited flow mode therapy regime may dictate a therapeutic level of a first gas parameter of the one or more gas parameters at or near the airway of the subject. In some examples, operation 208 is performed by a computer program module the same as or similar to control module 54 (shown in FIG. 1 and described herein).

[0047] At an operation 210, a compensation amount may be determined. The compensation amount may be an amount to adjust the first gas parameter to compensate for respiratory effort during inhalation to maintain the therapeutic level for the first gas parameter. Determining the compensation amount is based on the therapeutic level and the output signals. In some examples, operation 210 is performed by a computer program module the same as or similar to compensation module 56 (shown in FIG. 1 and described herein).

[0048] At an operation 212, the pressurized flow of breathable gas is controlled to reflect the compensation amount. Generation of the pressurized flow of breathable gas may be controlled such that the first gas parameter is maintained at a level that reflects the compensation amount. In some examples, operation 212 is performed by a computer program module the same as or similar to control module 54 (shown in FIG. 1 and described herein).

[0049] At an operation 214, a compensation limit may be determined. The compensation limit may be determined for the compensation amount of the first gas parameter. The compensation limit may be determined based on the current

leak value. In some examples, operation 214 is performed by a computer program module the same as or similar to compensation limit module 58 (shown in FIG. 1 and described herein).

[0050] At an operation 216, the compensation limit may be implemented. The compensation limit may be implemented as a limit for the compensation amount. In some examples, operation 216 is performed by a computer program module the same as or similar to compensation module 56 (shown in FIG. 1 and described herein).

[0051] In the claims, any reference signs placed between parentheses shall not be construed as limiting the claim. The word "comprising" or "including" does not exclude the presence of elements or steps other than those listed in a claim. In a device claim enumerating several means, several of these means may be embodied by one and the same item of hardware. The word "a" or "an" preceding an element does not exclude the presence of a plurality of such elements. In any device claim enumerating several means, several of these means may be embodied by one and the same item of hardware. The mere fact that certain elements are recited in mutually different dependent claims does not indicate that these elements cannot be used in combination.

[0052] Although the description provided above provides detail for the purpose of illustration based on what is currently considered to be the most practical and preferred embodiments, it is to be understood that such detail is solely for that purpose and that the disclosure is not limited to the expressly disclosed embodiments, but, on the contrary, is intended to cover modifications and equivalent arrangements that are within the scope of the appended claims.

Claims

1. A pressure support system (10) configured to deliver a pressurized flow of breathable gas to the airway of a subject (12), the pressure support system comprising:

a pressure generator (14) configured to generate the pressurized flow of breathable gas;
one or more sensors (18) configured to generate output signals conveying information related to one or more gas parameters of the pressurized flow of breathable gas; and
one or more processors (20) configured to execute computer program modules, the computer program modules comprising:

a leak module (52) configured to estimate a current leak value;
a control module (54) configured to control operation of the pressure generator to generate the pressurized flow of breathable gas according to a limited flow mode therapy regime that dictates a therapeutic level of a flow rate of the one or more gas parameters at or near the airway of the subject;
a compensation module (56) configured to determine a compensation amount to adjust the flow rate to compensate for respiratory effort during inhalation to maintain the therapeutic level for the flow rate, wherein the compensation module is configured to determine the compensation amount based on the therapeutic level and the output signals;
wherein the control module is configured to control the pressure generator to generate the pressurized flow of breathable gas with the flow rate at a level that reflects the compensation amount; and
a compensation limit module (58) configured to determine a compensation limit for the compensation amount of the flow rate based on the current leak value;
wherein the compensation module is configured to implement the compensation limit as a limit for the compensation amount, wherein the current leak value is an instantaneous indication of the amount of leak in the pressure support system (10), wherein the compensation limit module is configured to determine a flow rate compensation limit that is one to two times the current leak value.

Patentansprüche

1. Druckhaltesystem (10), das konfiguriert ist, um einen druckbeaufschlagten Atemgasstrom in den Atemweg eines Subjekts (12) zu leiten, wobei das Druckhaltesystem umfasst:

einen Druckerzeuger (14), der konfiguriert ist, um den druckbeaufschlagten Atemgasstrom zu erzeugen;
einen oder mehrere Sensoren (18), die konfiguriert sind, um Ausgangssignale zu erzeugen, die Informationen in Bezug auf einen oder mehrere Gasparameter des druckbeaufschlagten Atemgasstroms übermitteln; und
einen oder mehrere Prozessoren (20), die konfiguriert sind, um Computerprogrammmodule auszuführen, wobei die Computerprogrammmodule umfassen:

ein Leckagemodul (52), das konfiguriert ist, um einen aktuellen Leckagewert zu schätzen;
 ein Steuermodul (54), das konfiguriert ist, um den Betrieb des Druckerzeugers zu steuern, um den druckbeaufschlagten Atemgasstrom gemäß einem Therapiekonzept mit begrenztem Strömungsmodus zu erzeugen, das ein therapeutisches Niveau einer Strömungsrate des einen oder der mehreren Gasparameter am oder in der Nähe des Atemwegs des Subjekts vorschreibt;
 ein Kompensationsmodul (56), das konfiguriert ist, um eine Kompensationsmenge zu bestimmen, um die Strömungsrate einzustellen, um die Atmungsanstrengung während der Inhalation zu kompensieren, um das therapeutische Niveau für die Strömungsrate aufrechtzuerhalten, wobei das Kompensationsmodul konfiguriert ist, um die Kompensationsmenge basierend auf dem therapeutischen Niveau und den Ausgangssignalen zu bestimmen;
 wobei das Steuermodul konfiguriert ist, um den Druckerzeuger zu steuern, um den druckbeaufschlagten Atemgasstrom mit der Strömungsrate auf einem Niveau zu erzeugen, das die Kompensationsmenge widerspiegelt; und
 ein Kompensationsgrenzmodul (58), das konfiguriert ist, um eine Kompensationsgrenze für die Kompensationsmenge der Strömungsrate basierend auf dem aktuellen Leckagewert zu bestimmen;

wobei das Kompensationsmodul konfiguriert ist, um die Kompensationsgrenze als Begrenzung für die Kompensationsmenge zu implementieren, wobei der aktuelle Leckagewert eine Istwertanzeige der Leckagemenge im Druckhaltesystem (10) ist, wobei das Kompensationsgrenzmodul konfiguriert ist, um eine Strömungskompensationsgrenze zu bestimmen, die das Ein- bis Zweifache des aktuellen Leckagewertes beträgt.

Revendications

1. Système de support de pression (10) configuré pour délivrer un flux pressurisé de gaz respirable aux voies respiratoires d'un sujet (12), le système de support de pression comprenant :

un générateur de pression (14) configuré pour produire le flux pressurisé de gaz respirable ;
 un ou plusieurs capteurs (18) configurés pour produire des signaux de sortie transportant des informations liées à un ou plusieurs paramètres de gaz du flux pressurisé de gaz respirable ; et
 un ou plusieurs processeurs (20) configurés pour exécuter des modules de programme informatique, les modules de programme informatique comprenant :

un module de fuite (52) configuré pour évaluer une valeur de fuite courante ;
 un module de commande (54) configuré pour commander le fonctionnement du générateur de pression pour produire le flux pressurisé de gaz respirable selon un régime de thérapie en mode de flux limité qui dicte un niveau thérapeutique d'un débit du ou des plusieurs paramètres de gaz au niveau ou près des voies respiratoires du sujet ;
 un module de compensation (56) configuré pour déterminer une quantité de compensation pour ajuster le débit pour compenser un effort respiratoire pendant l'inhalation pour maintenir le niveau thérapeutique pour le débit, dans lequel le module de compensation est configuré pour déterminer la quantité de compensation sur la base du niveau thérapeutique et des signaux de sortie ;
 dans lequel le module de commande est configuré pour commander le générateur de pression pour produire le flux pressurisé de gaz respirable avec le débit à un niveau qui reflète la quantité de compensation ; et
 un module de limite de compensation (58) configuré pour déterminer une limite de compensation pour la quantité de compensation du débit sur la base de la valeur de fuite courante ;

dans lequel le module de compensation est configuré pour mettre en oeuvre la limite de compensation en tant que limite pour la quantité de compensation, dans lequel la valeur de fuite courante est une indication instantanée de la quantité de fuite dans le système de support de pression (10), dans lequel le module de limite de compensation est configuré pour déterminer une limite de compensation de débit qui est une à deux fois la valeur de fuite courante.

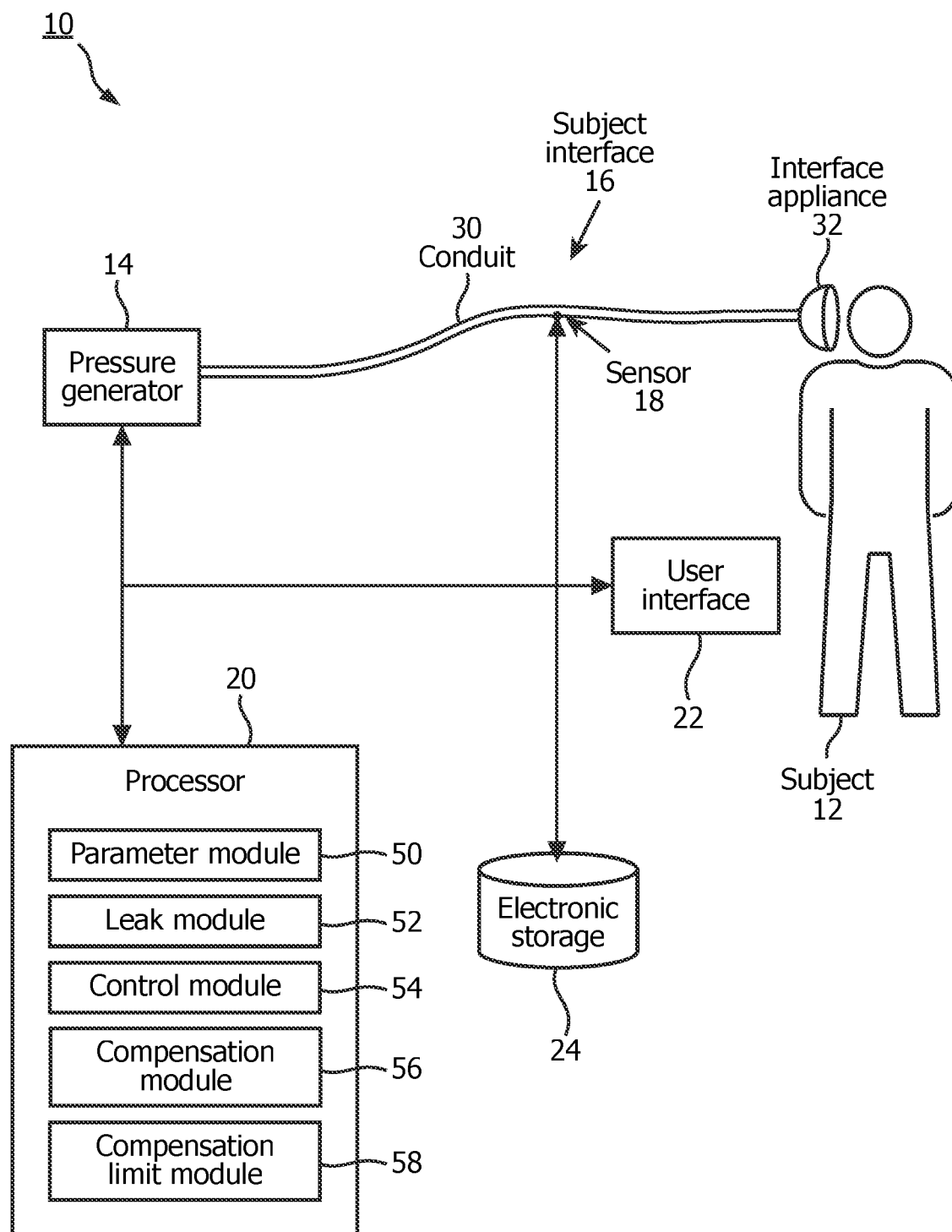


FIG. 1

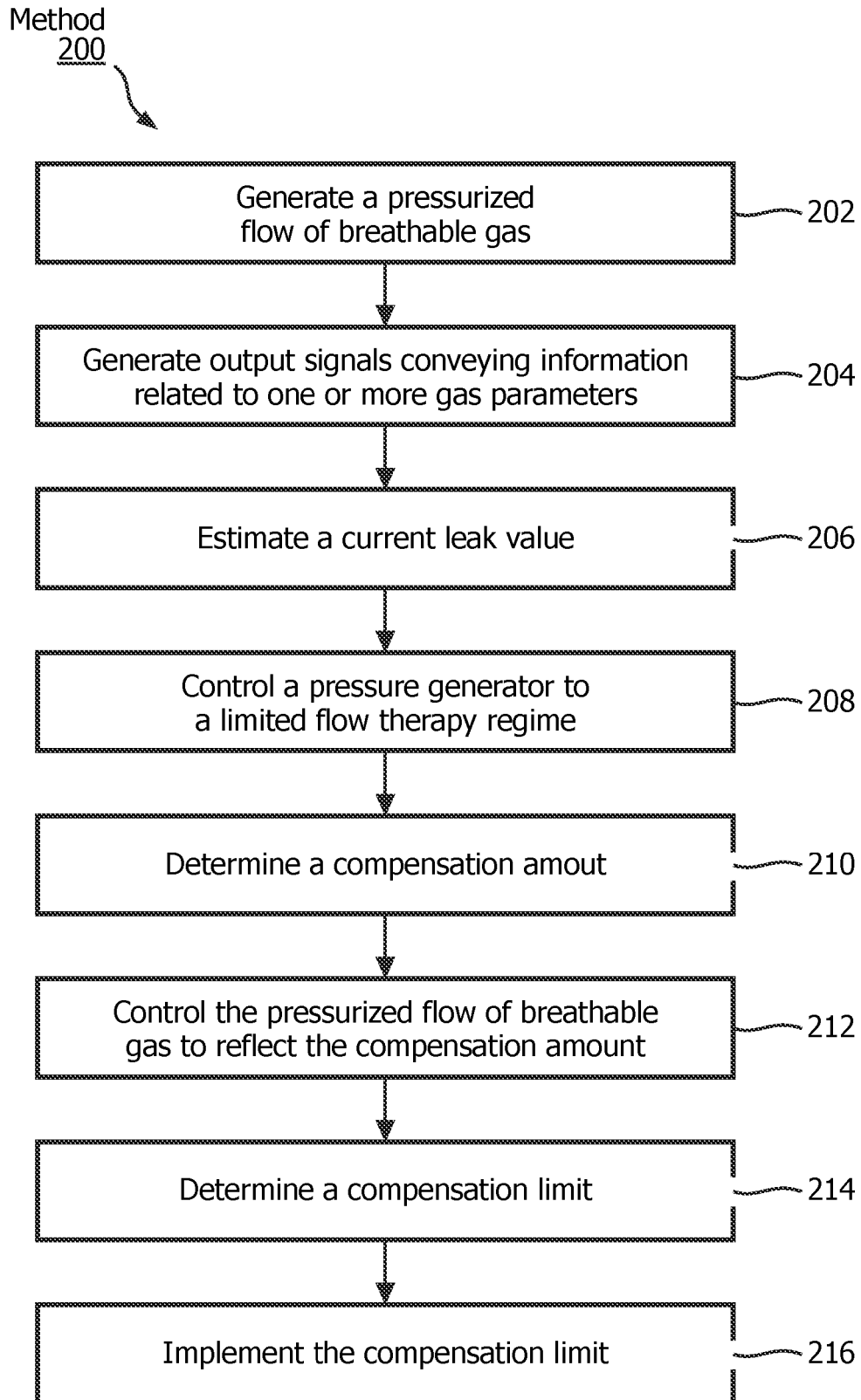


FIG. 2

REFERENCES CITED IN THE DESCRIPTION

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专利名称(译)	用于在限流呼吸治疗期间限制流量和/或压力补偿的系统和方法		
公开(公告)号	EP2938379A1	公开(公告)日	2015-11-04
申请号	EP2013830104	申请日	2013-12-17
[标]申请(专利权)人(译)	皇家飞利浦电子股份有限公司		
申请(专利权)人(译)	皇家飞利浦N.V.		
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IPC分类号	A61M16/00 A61B5/08 A61B5/087 A61B5/091 A61M16/04 A61M16/06 A61M16/08 A61B5/00 A61M16/10 A61M16/16 A61M16/20		
CPC分类号	A61B5/0816 A61B5/082 A61B5/087 A61B5/091 A61B5/4836 A61M16/0057 A61M16/0069 A61M16/024 A61M16/161 A61M16/201 A61M2016/0015 A61M2016/0027 A61M2016/003 A61M2016/102 A61M2205/15 A61M2205/3331 A61M2205/3365 A61M2205/3368 A61M2205/3375 A61M2205/502 A61M2205/52 A61M16/0003		
代理机构(译)	STEFFEN , THOMAS		
优先权	61/745870 2012-12-26 US		
其他公开文献	EP2938379B1		
外部链接	Espacenet		

摘要(译)

描述了一种压力支撑系统，该压力支撑系统构造成为将加压的可呼吸气体流输送到受试者的气道。该系统被配置为以有限的流量呼吸疗法和/或其他疗法来治疗阻塞性睡眠呼吸暂停，其他睡眠呼吸紊乱和/或其他呼吸问题。例如，限流呼吸疗法可以替代CPAP。该系统被配置为在吸气期间将流速补偿，压力补偿和/或发电机或其他参数的补偿限制为与电流泄漏成比例的值，以实现有限的流量呼吸治疗。在一些实施例中，该系统包括压力发生器，对象接口，一个或多个传感器，处理器，用户接口，电子存储器和/或其他组件中的一个或多个。