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(54) **FAST RECOVERY OF ECG SIGNAL METHOD AND APPARATUS**

(57) Fast recovery electrocardiogram (ECG) signal method and apparatus are provided. In one embodiment, an ECG apparatus includes an input for receiving a biometric cardiogram signal, such as a Wilson Central Terminal (WCT) signal, and a combiner, such as an adder, for producing a compensated signal. An analog to digital converter provides a digitized version of the compensated signal to a processor. The processor produces an ECG reflective of the compensated signal and also outputs a digital signal corresponding to high frequency re-

sponse of the digitized compensated signal to a digital to analog converter. The digital to analog converter provides an analog version of the digital signal corresponding to high frequency response of the digitized compensated signal to compensate for low response of the biometric cardiogram signal to high frequency spikes. A resultant ECG is produced by the processor having pacing signal contribution within the biometric cardiogram signal cancelled.

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Description

SUMMARY

[0001] Fast recovery electrocardiogram (ECG) signal method and apparatus are provided. In one embodiment, an ECG apparatus includes an input for receiving a biometric cardiogram signal of a patient and a compensation signal combiner for selectively producing a compensated biometric cardiogram signal of the biometric cardiogram signal of the patient. An analog to digital converter provides a digitized version of the compensated biometric cardiogram signal to a digital processor. The digital processor produces an ECG reflective of the compensated biometric cardiogram signal and also outputs a digital signal corresponding to high frequency response of the digitized compensated biometric cardiogram signal to a digital to analog converter. The digital to analog converter provides an analog version of the digital signal corresponding to high frequency response of the digitized compensated biometric cardiogram signal to the compensation signal combiner to compensate for low response of the biometric cardiogram signal of the patient to high frequency spikes. A resultant ECG is produced by the digital processor having pacing signal contribution within the biometric cardiogram signal cancelled.

[0002] Preferably, the input is configured to receive a Wilson Central Terminal (WCT) biometric cardiogram signal of a patient. Also, the compensation signal combiner is in one embodiment an adder. The compensated biometric cardiogram signal of the biometric cardiogram signal of the patient can be combined via an operational amplifier with an intra cardiac signal in a differential amplifier configuration as the input to the analog to digital converter. The processor can be configured to produce the ECG reflective of the compensated biometric cardiogram signal in a graph form reflecting microvolts of signal over time in tenths of seconds.

[0003] In another embodiment, a method of producing an electrocardiogram (ECG) is provided. A biometric cardiogram signal of a patient is received. A compensated biometric cardiogram signal of the biometric cardiogram signal of the patient is selectively produced. A digitized version of the compensated biometric cardiogram signal is provided to a digital processor. The digital processor produces an ECG reflective of the compensated biometric cardiogram signal and outputs a digital signal corresponding to high frequency response of the digitized compensated biometric cardiogram signal to a digital to analog converter. The digital to analog converter providing an analog version of the digital signal corresponding to high frequency response of the digitized compensated biometric cardiogram signal that is combined with the biometric cardiogram signal to compensate for low response of the biometric cardiogram signal of the patient to high frequency spikes. A resultant ECG is produced by the digital processor having pacing signal contribution within the biometric cardiogram signal cancelled.

[0004] Preferably, a Wilson Central Terminal (WCT) biometric cardiogram signal is received as the biometric cardiogram signal of the patient. Also, the analog version of the digital signal corresponding to high frequency response of the digitized compensated biometric cardiogram signal is in one embodiment added to biometric cardiogram signal produce the compensated biometric cardiogram signal.

[0005] The compensated biometric cardiogram signal of the biometric cardiogram signal of the patient can be combined via an operational amplifier with an intra cardiac signal in a differential amplifier configuration as the input to an analog to digital converter which provides the digitized version of the compensated biometric cardiogram signal to the digital processor. The processor can produce the ECG reflective of the compensated biometric cardiogram signal in a graph form reflecting microvolts of signal over time in tenths of seconds.

[0006] Other object and advantages of the invention will be apparent to those skilled in the art from the drawings and following detailed description.

BRIEF DESCRIPTION OF THE DRAWINGS

[0007]

Fig. 1 is a schematic illustration of an ECG system based on conventional teachings.

Fig. 2 is a schematic illustration of an ECG system in accordance with the teachings of the present invention.

Figs. 3(A)-3(C) are illustrations of ECG related signals.

Fig. 4 is a flow diagram of a method of producing an electrocardiogram (ECG) in accordance with the teachings of the present invention.

DETAILED DESCRIPTION OF THE PREFERRED EMBODIMENT(S)

[0008] The present invention is related to ECG systems and methods. The inventors have recognized that electrophysiology physicians require an enhanced ECG system that compensates for the interfering signals caused by pacing.

[0009] ECG monitoring systems that include pace pulse detection are known in the art. For example, see US Patent 5,682,902 (Herleikson). Such standard ECG input systems utilize analog to digital signal processing. Pacing signals can be detected through the analysis of the digital signals. In conventional ECG systems, such as Herleikson, pace pulse signals can be removed though replacement with a selected flat signal for a specified or calculated time. The inventors have recognized that electrophysiology physicians can benefit from an enhanced ECG system that more accurately compensates for the interfering signals caused by pacing.

[0010] Consistent with the conventional methodology,

an ECG system 10 can be constructed, for example, to process Wilson Central Terminal ("WCT") ECG signals of a patient that average three active limb electrode voltages measured with respect to a return ground electrode. As illustrated in Fig. 1, a WCT signal can be combined via an operational amplifier 12 with an intra cardiac signal 14 in a differential amplifier configuration 15 as the input to an analog to digital converter 16. The digital output of the analog to digital converter 16 is then processed by a processor 18 in a conventional manner, such as corresponding to the processing taught by Herleikson, to produce an ECG corresponding to the WCT signal.

[0011] When the WCT signal includes a pacing charge, however, the ECG produced by the system 10 that uses conventional processing of the digitized signal, is partially skewed due to conventional processing of the pacing signal.

[0012] The present invention provides an improved ECG system that implements a digital to analog compensation value to cancel out the pacing charge such that a more accurate ECG is produced. Referring to Fig. 2, an example fast-recovery ECG input system 20 is provided that utilizes an analog to digital converter 16 and associated processor 18 to detect pacing, similar to the system 10 of Fig. 1. However, the processor 18 of the Fig. 2 modified system 20 is configured to process the WCT signal after being combined with an added DC value signal 21 that cancels out the pacing charge when the WCT signal includes a pacing charge.

[0013] Applicants have recognized that when a pacing signal is applied, the WCT signal will include both significant low and high frequency components that arise from the electronic pacing pulse. As illustrated in Figure 2, the WCT signal is passed through an adder 22 which adds the cancellation signal 21 to compensate for the low response of the WCT signal to high frequency spikes. The post-adder "compensated" WCT signal 23 is provided to the analog to digital converter 16 via the operational amplifier 12 with an intra cardiac signal 14 in a differential amplifier configuration 15. The digital output of the analog to digital converter 16 is then provided to a digital processor 18.

[0014] The digital output of the analog to digital converter 16 is processed by the processor 18 in a conventional manner, such as corresponding to the processing taught by Herleikson, to produce an ECG corresponding to the compensated WCT signal. Additionally, however, a high frequency response of the digital signal received from the analog to digital converter 16 is used by the processor 18 to create a digital compensation signal 25. The digital compensation signal 25 is passed through a digital to analog converter 24 to provide the analog signal 21 which is added to the WCT signal. The result of adding the cancellation signal 21 to the WCT signal causes the processor 18 to produce an ECG having the pacing signal contribution within the biometric cardiogram signal cancelled since the ECG is based on the compensated WCT signal 23.

[0015] The high frequency response of the WCT signal, which is significant when the WCT signal includes a pacing pulse, is determined by the processor 18 to produce the digital compensation signal 25 that is fed to the digital to analog converter 24 to provide the compensation signal 21 which is added to the WCT signal. Once a pacing artifact is detected by the processor 18, a short averaging window can be used to keep the signal always without an offset. The digital compensation signal 25 input to the digital to analog converter 24 is smoothed to avoid steps.

[0016] The resultant ECG signal graphs both with and without having the cancellation signal applied are illustrated in Figs. 3A and C. Fig. 3A reflects the WCT signal without cancellation and Fig. 3C illustrates the resultant ECG that utilizes the pace pulse cancellation of the fast-recovery ECG input system 20. For reference, Fig. 3B is provided that reflects an ECG channel response to a pace pulse signal within the WCT signal. The graphs reflect microvolts (μ Vs) of signal over one second of time.

[0017] With reference to Fig. 4, An example method of producing the ECG depicted in Fig. 3C is provided. In step 41, a biometric cardiogram signal of a patient is received. In step 43, a compensated biometric cardiogram signal is produced by adding an analog compensation signal to the biometric cardiogram signal of the patient. In step 45, a digitized version of the compensated biometric cardiogram signal is provided to a digital processor. In step 47, the digital processor produces an ECG reflective of the compensated biometric cardiogram signal and outputs a digital signal corresponding to high frequency response of the digitized compensated biometric cardiogram signal to a digital to analog converter. In step 49, the digital to analog converter provides an analog version of the digital signal corresponding to high frequency response of the digitized compensated biometric cardiogram signal that is combined with the biometric cardiogram signal in step 43 to compensate for low response of the biometric cardiogram signal of the patient to high frequency spikes whereby an ECG is produced by the digital processor having pacing signal contribution within the biometric cardiogram signal cancelled.

[0018] All references cited in this application are incorporated by reference herein as if fully set forth. It will be apparent to one of ordinary skill in the art that many changes and modifications can be made to the embodiments described without departing from the spirit or scope of the invention as set forth herein.

ASPECTS OF THE INVENTION

[0019]

1. An electrocardiogram (ECG) apparatus comprising:

an input for receiving a biometric cardiogram sig-

- nal of a patient;
 a compensation signal combiner for selectively producing a compensated biometric cardiogram signal of the biometric cardiogram signal of the patient;
 an analog to digital converter for providing a digitized version of the compensated biometric cardiogram signal to a digital processor;
 the digital processor configured to produce an ECG reflective of the compensated biometric cardiogram signal and to output a digital signal corresponding to high frequency response of the digitized compensated biometric cardiogram signal to a digital to analog converter; and
 the digital to analog converter configured to provide an analog version of the digital signal corresponding to high frequency response of the digitized compensated biometric cardiogram signal to the compensation signal combiner to compensate for low response of the biometric cardiogram signal of the patient to high frequency spikes whereby an ECG is produced by the digital processor having pacing signal contribution within the biometric cardiogram signal cancelled.
2. The ECG apparatus according to aspect 1 wherein the input is configured to receive a Wilson Central Terminal (WCT) biometric cardiogram signal of a patient.
3. The ECG apparatus according to aspect 2 wherein the compensation signal combiner is an adder.
4. The ECG apparatus according to aspect 3 wherein the compensated biometric cardiogram signal of the biometric cardiogram signal of the patient is combined via an operational amplifier with an intra cardiac signal in a differential amplifier configuration as the input to the analog to digital converter.
5. The ECG apparatus according to aspect 4 wherein the processor produces the ECG reflective of the compensated biometric cardiogram signal in a graph form reflecting microvolts of signal over time in tenths of seconds.
6. The ECG apparatus according to aspect 1 wherein the compensation signal combiner is an adder.
7. The ECG apparatus according to aspect 6 wherein the compensated biometric cardiogram signal of the biometric cardiogram signal of the patient is combined via an operational amplifier with an intra cardiac signal in a differential amplifier configuration as the input to the analog to digital converter.
8. The ECG apparatus according to aspect 7 wherein
- the processor produces the ECG reflective of the compensated biometric cardiogram signal in a graph form reflecting microvolts of signal over time in tenths of seconds.
9. The ECG apparatus according to aspect 1 wherein the compensated biometric cardiogram signal of the biometric cardiogram signal of the patient is combined via an operational amplifier with an intra cardiac signal in a differential amplifier configuration as the input to the analog to digital converter.
10. The ECG apparatus according to aspect 9 wherein the processor produces the ECG reflective of the compensated biometric cardiogram signal in a graph form reflecting microvolts of signal over time in tenths of seconds.
11. A method of producing an electrocardiogram (ECG) comprising:
- receiving a biometric cardiogram signal of a patient;
 - selectively producing a compensated biometric cardiogram signal of the biometric cardiogram signal of the patient;
 - providing a digitized version of the compensated biometric cardiogram signal to a digital processor;
 - the digital processor producing an ECG reflective of the compensated biometric cardiogram signal and outputting a digital signal corresponding to high frequency response of the digitized compensated biometric cardiogram signal to a digital to analog converter; and
 - the digital to analog converter providing an analog version of the digital signal corresponding to high frequency response of the digitized compensated biometric cardiogram signal that is combined with the biometric cardiogram signal to compensate for low response of the biometric cardiogram signal of the patient to high frequency spikes whereby an ECG is produced by the digital processor having pacing signal contribution within the biometric cardiogram signal cancelled.
12. The method according to aspect 11 wherein a Wilson Central Terminal (WCT) biometric cardiogram signal is received as the biometric cardiogram signal of the patient.
13. The method according to aspect 12 wherein the analog version of the digital signal corresponding to high frequency response of the digitized compensated biometric cardiogram signal is added to biometric cardiogram signal produce the compensated biometric cardiogram signal.

14. The method according to aspect 13 wherein the compensated biometric cardiogram signal of the biometric cardiogram signal of the patient is combined via an operational amplifier with an intra cardiac signal in a differential amplifier configuration as the input to an analog to digital converter which provides the digitized version of the compensated biometric cardiogram signal to the digital processor.

15. The method according to aspect 14 wherein the processor produces the ECG reflective of the compensated biometric cardiogram signal in a graph form reflecting microvolts of signal over time in tenths of seconds.

16. The method according to aspect 11 wherein the analog version of the digital signal corresponding to high frequency response of the digitized compensated biometric cardiogram signal is added to biometric cardiogram signal produce the compensated biometric cardiogram signal.

17. The method according to aspect 16 wherein the compensated biometric cardiogram signal of the biometric cardiogram signal of the patient is combined via an operational amplifier with an intra cardiac signal in a differential amplifier configuration as the input to an analog to digital converter which provides the digitized version of the compensated biometric cardiogram signal to the digital processor.

18. The method according to aspect 17 wherein the processor produces the ECG reflective of the compensated biometric cardiogram signal in a graph form reflecting microvolts of signal over time in tenths of seconds.

19. The method according to aspect 11 wherein the compensated biometric cardiogram signal of the biometric cardiogram signal of the patient is combined via an operational amplifier with an intra cardiac signal in a differential amplifier configuration as the input to an analog to digital converter which provides the digitized version of the compensated biometric cardiogram signal to the digital processor.

20. The method according to aspect 19 wherein the processor produces the ECG reflective of the compensated biometric cardiogram signal in a graph form reflecting microvolts of signal over time in tenths of seconds.

Claims

1. An electrocardiogram (ECG) apparatus comprising:
an input for receiving a biometric cardiogram sig-

nal of a patient;
a compensation signal combiner for selectively producing a compensated biometric cardiogram signal of the biometric cardiogram signal of the patient;
an analog to digital converter for providing a digitized version of the compensated biometric cardiogram signal to a digital processor;
the digital processor configured to produce an ECG reflective of the compensated biometric cardiogram signal and to output a digital signal corresponding to high frequency response of the digitized compensated biometric cardiogram signal to a digital to analog converter; and
the digital to analog converter configured to provide an analog version of the digital signal corresponding to high frequency response of the digitized compensated biometric cardiogram signal to the compensation signal combiner to compensate for low response of the biometric cardiogram signal of the patient to high frequency spikes whereby an ECG is produced by the digital processor having pacing signal contribution within the biometric cardiogram signal cancelled.

- 2. The ECG apparatus according to claim 1 wherein the input is configured to receive a Wilson Central Terminal (WCT) biometric cardiogram signal of a patient.
- 3. The ECG apparatus according to claim 2 wherein the compensation signal combiner is an adder.
- 4. The ECG apparatus according to claim 1 wherein the compensation signal combiner is an adder.
- 5. The ECG apparatus according to claim 1, 3 or 4 wherein the compensated biometric cardiogram signal of the biometric cardiogram signal of the patient is combined via an operational amplifier with an intra cardiac signal in a differential amplifier configuration as the input to the analog to digital converter.
- 6. The ECG apparatus according to claim 5 wherein the processor produces the ECG reflective of the compensated biometric cardiogram signal in a graph form reflecting microvolts of signal over time in tenths of seconds.
- 7. A method of producing an electrocardiogram (ECG) comprising:

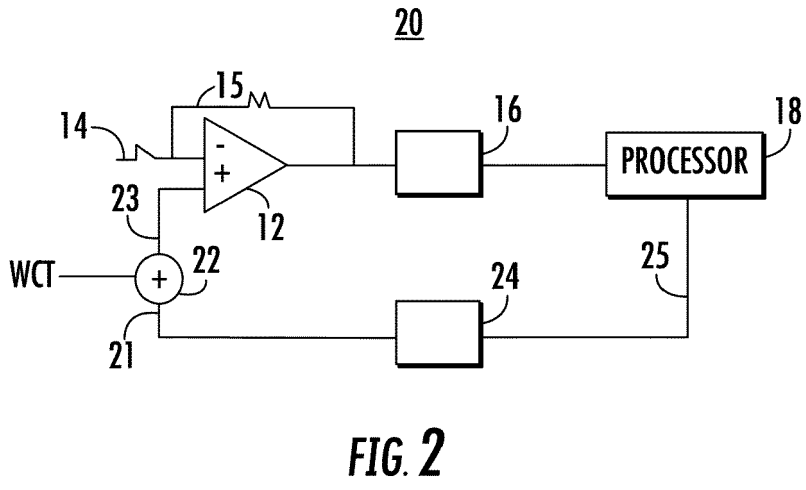
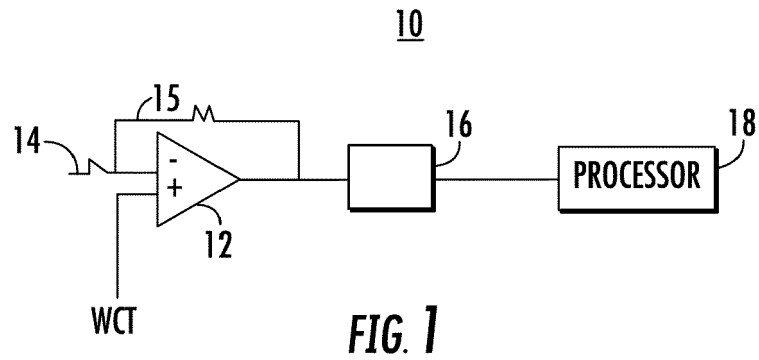
receiving a biometric cardiogram signal of a patient;
selectively producing a compensated biometric cardiogram signal of the biometric cardiogram signal of the patient;

providing a digitized version of the compensated biometric cardiogram signal to a digital processor;
 the digital processor producing an ECG reflective of the compensated biometric cardiogram signal and outputting a digital signal corresponding to high frequency response of the digitized compensated biometric cardiogram signal to a digital to analog converter; and
 the digital to analog converter providing an analog version of the digital signal corresponding to high frequency response of the digitized compensated biometric cardiogram signal that is combined with the biometric cardiogram signal to compensate for low response of the biometric cardiogram signal of the patient to high frequency spikes whereby an ECG is produced by the digital processor having pacing signal contribution within the biometric cardiogram signal cancelled.

- 8. The method according to claim 7 wherein a Wilson Central Terminal (WCT) biometric cardiogram signal is received as the biometric cardiogram signal of the patient.
- 9. The method according to claim 7 or claim 8 wherein the analog version of the digital signal corresponding to high frequency response of the digitized compensated biometric cardiogram signal is added to biometric cardiogram signal produce the compensated biometric cardiogram signal.
- 10. The method according to claim 7 or claim 9 wherein the compensated biometric cardiogram signal of the biometric cardiogram signal of the patient is combined via an operational amplifier with an intra cardiac signal in a differential amplifier configuration as the input to an analog to digital converter which provides the digitized version of the compensated biometric cardiogram signal to the digital processor.
- 11. The method according to claim 10 wherein the processor produces the ECG reflective of the compensated biometric cardiogram signal in a graph form reflecting microvolts of signal over time in tenths of seconds.

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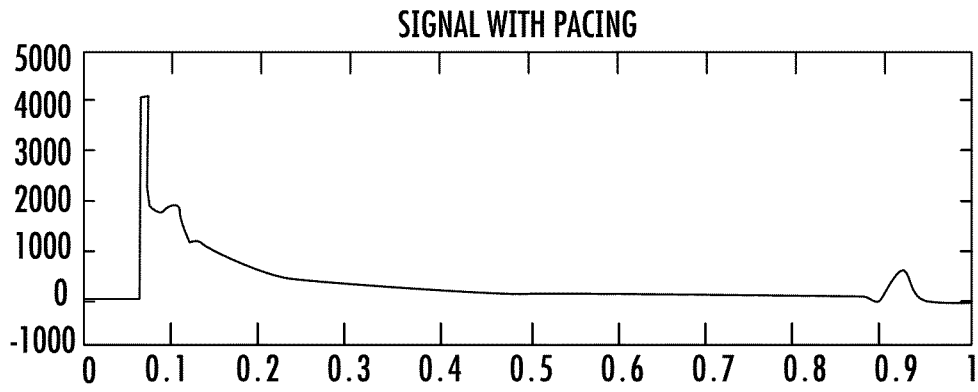


FIG. 3A

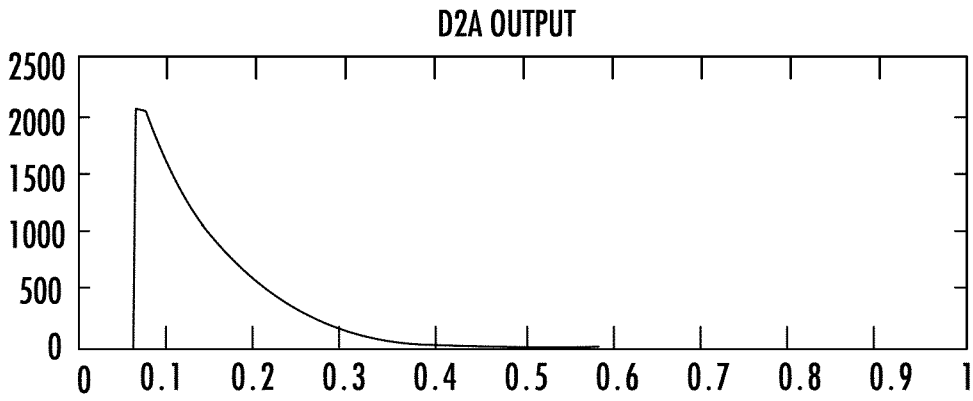


FIG. 3B

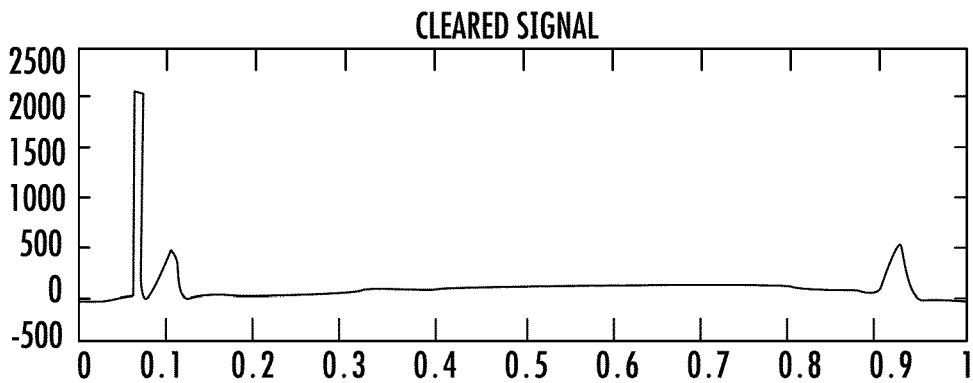


FIG. 3C

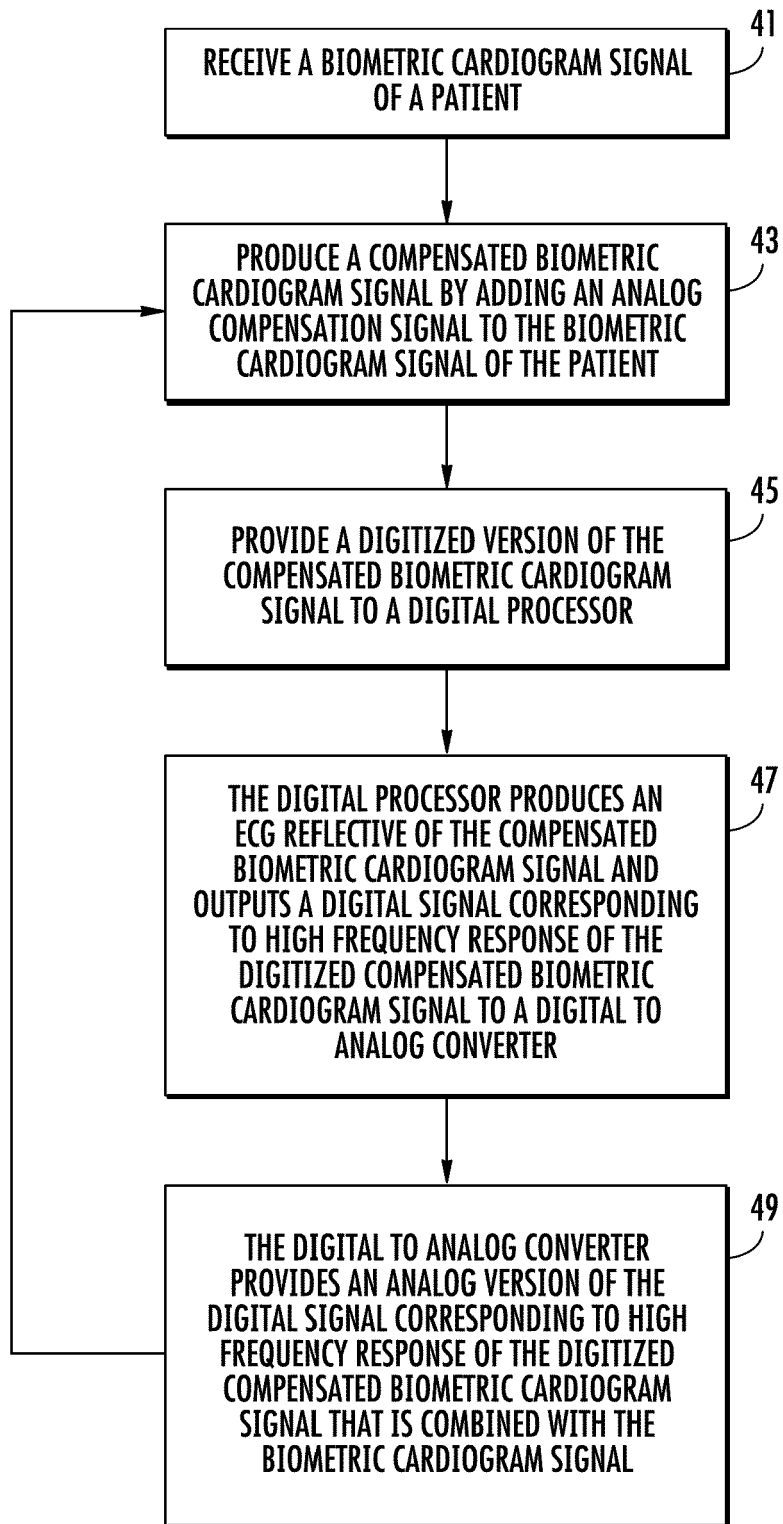


FIG. 4



EUROPEAN SEARCH REPORT

Application Number
EP 18 20 9055

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DOCUMENTS CONSIDERED TO BE RELEVANT			
Category	Citation of document with indication, where appropriate, of relevant passages	Relevant to claim	CLASSIFICATION OF THE APPLICATION (IPC)
X	US 5 205 294 A (FLACH TERRY E [US] ET AL) 27 April 1993 (1993-04-27) * column 5, line 33 - column 6, line 25 * * column 9, line 43 - column 10, line 47 * * figures 1,5,6 *	1-11	INV. A61B5/0428
A	----- WO 2013/103353 A1 (DRAEGER MEDICAL SYSTEMS INC [US]; QIN DEREK YONG [US]; MAURER DAVID CH) 11 July 2013 (2013-07-11) * page 4, line 1 - page 9, line 13 * * figure 1 *	1-11	ADD. A61B5/00 A61B5/042
A,D	----- US 5 682 902 A (HERLEIKSON EARL C [US]) 4 November 1997 (1997-11-04) * the whole document *	1-11	

The present search report has been drawn up for all claims			
Place of search The Hague		Date of completion of the search 20 February 2019	Examiner Bataille, Frédéric
CATEGORY OF CITED DOCUMENTS X : particularly relevant if taken alone Y : particularly relevant if combined with another document of the same category A : technological background O : non-written disclosure P : intermediate document		T : theory or principle underlying the invention E : earlier patent document, but published on, or after the filing date D : document cited in the application L : document cited for other reasons & : member of the same patent family, corresponding document	

EPO FORM 1503 03/02 (P04C01)

**ANNEX TO THE EUROPEAN SEARCH REPORT
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EP 18 20 9055

5 This annex lists the patent family members relating to the patent documents cited in the above-mentioned European search report.
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20-02-2019

Patent document cited in search report	Publication date	Patent family member(s)	Publication date
US 5205294 A	27-04-1993	NONE	

WO 2013103353 A1	11-07-2013	EP 2800508 A1	12-11-2014
		US 2014336948 A1	13-11-2014
		WO 2013103353 A1	11-07-2013

US 5682902 A	04-11-1997	DE 19637876 A1	17-04-1997
		GB 2306661 A	07-05-1997
		JP 3982856 B2	26-09-2007
		JP H09164122 A	24-06-1997
		US 5682902 A	04-11-1997

EPO FORM P0459

For more details about this annex : see Official Journal of the European Patent Office, No. 12/82

REFERENCES CITED IN THE DESCRIPTION

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Patent documents cited in the description

- US 5682902 A, Herleikson **[0009]**

专利名称(译)	心电信号的快速恢复方法和装置		
公开(公告)号	EP3492007A1	公开(公告)日	2019-06-05
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申请(专利权)人(译)	生物传感韦伯斯特(以色列)LTD.		
当前申请(专利权)人(译)	生物传感韦伯斯特(以色列)LTD.		
[标]发明人	GOVARI ASSAF		
发明人	GOVARI, ASSAF		
IPC分类号	A61B5/0428 A61B5/00 A61B5/042		
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外部链接	Espacenet		

摘要(译)

提供了快速恢复心电图 (ECG) 信号方法和装置。在一个实施例中，ECG设备包括用于接收生物测定心电图信号的输入，例如Wilson中心终端 (WCT) 信号，以及用于产生补偿信号的组合器，例如加法器。模数转换器向处理器提供补偿信号的数字化版本。处理器产生反映补偿信号的ECG，并且还将对应于数字化补偿信号的高频响应的数字信号输出到数模转换器。数模转换器提供对应于数字化补偿信号的高频响应的数字信号的模拟版本，以补偿生物测定心电图信号对高频尖峰的低响应。由处理器产生得到的ECG，其中消除了生物测定心电图信号内的起搏信号贡献。

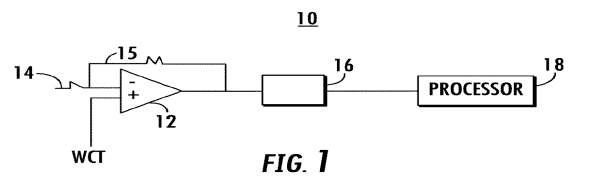


FIG. 1

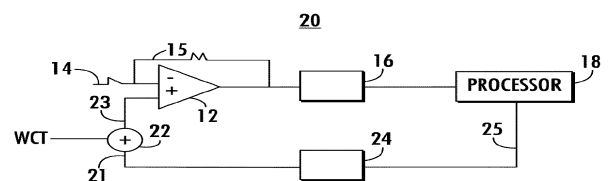


FIG. 2