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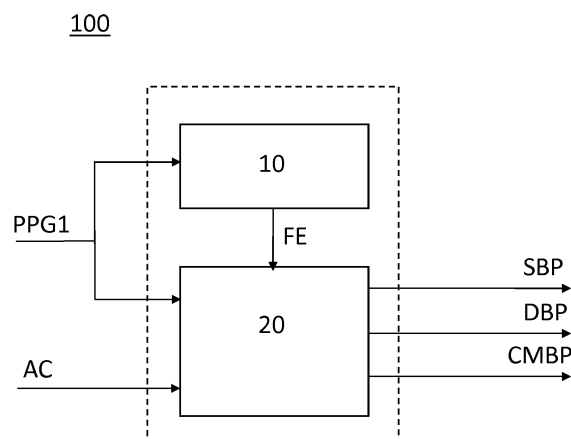
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(54) **SYSTEM AND METHOD FOR BLOOD PRESSURE ESTIMATION**

(57) An electronic system (100) for estimating a subject's blood pressure, comprising: a feature extraction module (10) configured for receiving a subject's photoplethysmogram signal (PPG1), detecting a plurality of signal characteristic points on said received photoplethysmogram signal (PPG1), calculating a plurality of distances in both time and amplitude between any two of said detected photoplethysmogram signal characteristic points, and providing a feature information signal (FE) comprising information about said calculated distances; and a blood pressure calculation module (20) configured for receiving said photoplethysmogram signal (PPG1), said feature information signal (FE) and anthropometric characteristics (AC) of the subject, and the blood pressure calculation module (20) comprising a first estimation

module (21) configured for calculating systolic and diastolic blood pressure values (SBP, DBP) of the subject based on said received feature information signal (FE) and anthropometric characteristics (AC), and a second estimation module (25) configured for calculating continuous mean blood pressure values (CMBP) of the subject based on said calculated systolic and diastolic blood pressure values (SBP, DBP) and said photoplethysmogram signal (PPG1); and wherein the first estimation module (21) uses a machine-learning regression model for calculating said systolic and diastolic blood pressure values (SBP, DBP) and the second estimation module (25) uses a Hilbert-Huang transform and an empirical mode decomposition process for calculating said continuous mean blood pressure values (CMBP).

Figure 1



Description**Technical Field**

- 5 **[0001]** The present description relates generally to electronic systems for arterial blood pressure estimation and more specifically to an electronic system, device and method for non-invasive, cuffless blood pressure estimation.

Background

- 10 **[0002]** Continuous and non-invasive estimation of arterial blood pressure (BP) without using a cuff has gained emerging interest for health care applications. Instead of commonly used cuff-based measurements, changes in the Pulse Wave Velocity (PWV), i.e., the speed of a pressure pulse propagating along the arterial wall, can be an alternative approach for a continuous, non-invasive and indirect BP measurement, as for example described in "Continuous blood pressure measurement by using the pulse transit time: comparison to a cuff-based method", by H. Gesche et al., European Journal of Applied Physiology, vol.112, no.1, pp.309-315, 2012, Springer-Verlag. PWV depends both on the arterial pressure and the intrinsic elastic properties of the arterial wall. Although this relationship is very well defined in a theoretical framework, it is practically difficult to have an accurate estimate of the relationship between PWV and BP since external factors like ageing with its related diseases, cardiovascular risk factors and others can significantly influence arterial wall stiffness.
- 20 **[0003]** As a surrogate of PWV, an indirect estimation of BP can be also obtained with the use of Pulse Transit Time (PTT), i.e., the time delay between the R-wave of the ECG and the arrival of the pulse wave measured in a peripheral position, as for example described in "Wearable Cuff-less PTT-based System for Overnight Blood Pressure Monitoring", by Yali Zheng et al., Engineering in Medicine and Biology Society (EMBS), 35th Annual International Conference of the IEEE EMBS, pp.6103-6106, Osaka 3-7 July 2013.
- 25 **[0004]** There is a motivation to improve current state of the art electronic systems and methods for non-invasive, cuffless blood pressure estimation.

Summary

- 30 **[0005]** A new and improved system and method for non-invasive, cuffless blood pressure estimation is herein proposed, which calculates the systolic, diastolic and/or continuous mean arterial blood pressure of a living being subject.
- [0006]** According to an exemplary embodiment, the system is able to calculate the arterial blood pressure of the subject over time, by gathering data about the subject's variations in blood volume. This is advantageous since the system is able to monitor the blood pressure level continuously during a certain lifetime period of the subject in a non-invasively manner and without affecting the daily normal activities of that living being subject.
- 35 **[0007]** According to an exemplary embodiment, there is provided a an electronic system for estimating a subject's blood pressure, comprising: a feature extraction module configured for receiving a subject's photoplethysmogram signal, detecting a plurality of signal characteristic points on said received photoplethysmogram signal, calculating a plurality of distances in both time and amplitude between any two of said detected photoplethysmogram signal characteristic points, and providing a feature information signal comprising information about said calculated distances; and a blood pressure calculation module configured for receiving said photoplethysmogram signal, said feature information signal and anthropometric characteristics of the subject, and the blood pressure calculation module comprising a first estimation module configured for calculating systolic and diastolic blood pressure values of the subject based on said received feature information signal and anthropometric characteristics, and a second estimation module configured for calculating continuous mean blood pressure values of the subject based on said calculated systolic and diastolic blood pressure values and said photoplethysmogram signal; and wherein the first estimation module uses a machine-learning regression model for calculating said systolic and diastolic blood pressure values and the second estimation module uses a Hilbert-Huang transform and an empirical mode decomposition process for calculating said continuous mean blood pressure values.
- 40 **[0008]** According to an exemplary embodiment, the feature extraction module is further configured generate at least one probabilistic distribution of the calculated distances and provide this information, as a feature information signal, to the blood pressure calculation module.
- [0009]** According to an exemplary embodiment, the first estimation module is trained using mathematical models that, from examples of photoplethysmogram signals, anthropometric characteristics and systolic and diastolic blood pressure values from a plurality of subjects, learn the association between the feature vectors computed in the feature extraction module and the corresponding systolic and diastolic blood pressure values.
- 55 **[0010]** According to an exemplary embodiment, the feature extraction module is further configured for receiving a subject's electrocardiogram signal, detecting a plurality of signal characteristic point on said received electrocardiogram

signal, calculating a plurality of distances in both time and amplitude between any two of said detected electrocardiogram signal characteristic points and between any point of said detected electrocardiogram signal characteristic points and any point of said photoplethysmogram signal characteristic points, and providing a feature information signal comprising information about said calculated distances; and the first estimation module is further configured for using mathematical models that express the relation between the summarized characteristic point distances of said electrocardiogram signal, said photoplethysmogram signal and a combination of both, the anthropometric characteristics and the arterial blood pressure levels of the subject.

[0011] According to an exemplary embodiment, the first estimation module is trained using a linear and/or multiple linear regression model, a random forest regression model, a Bayesian model and/or general machine learning regression model.

[0012] According to an exemplary embodiment, the machine-learning regression model is a discretized version of a regression model.

[0013] According to an exemplary embodiment, the regression module is trained using a linear and/or multiple linear classification and regression model, a random forest classification and regression model, a Bayesian model and/or general machine learning-based classification and regression model.

[0014] The invention also relates to an electronic device comprising a system for estimating a subject's blood pressure according to embodiments herein described.

[0015] The invention also relates to a method for estimating a subject's blood pressure comprising: receiving a subject's photoplethysmogram signal and anthropometric characteristics; detecting a plurality of signal characteristic points on said received photoplethysmogram signal; calculating a plurality of distances in both time and amplitude between any two of said detected photoplethysmogram signal characteristic points; calculating, based on said calculated distances and said anthropometric characteristics, said subject's systolic and diastolic blood pressure values using a machine-learning regression model; and calculating, based on said received systolic and diastolic blood pressure values and photoplethysmogram signal, said subject's continuous mean blood pressure values using a Hilbert-Huang transform and an empirical mode decomposition process.

[0016] According to an exemplary embodiment, the method further comprises receiving a subject's electrocardiogram signal; detecting a plurality of signal characteristic points on said received electrocardiogram signal; and calculating a plurality of distances in both time and amplitude between any two of said detected electrocardiogram signal characteristic points and between any of said detected electrocardiogram signal characteristic points and any of said photoplethysmogram signal characteristic points.

[0017] The invention also relates to a computer program product comprising computer program code means adapted to calculate a subject's blood pressure according to the methods herein described when said program is run on a computer, and to a computer readable storage medium comprising such computer program.

[0018] According to an exemplary embodiment, there is provided a system for estimating a subject's blood pressure, comprising a feature extraction module configured for receiving a subject's photoplethysmogram (PPG) signal, detect a plurality of signal characteristic points on said received PPG signal, calculate a plurality of possible pair-wise distances in both time and amplitude between said detected PPG signal characteristic points, and providing a feature information signal comprising information about said calculated distances; and a blood pressure calculation module configured for receiving said PPG signal, said feature information signal and anthropometric characteristics of that subject; and said blood pressure calculation module comprising a regression module configured for calculating said subject's systolic and diastolic blood pressure values using a machine-learning regression model and based on said received feature information signal and anthropometric characteristics; and an empirical mode decomposition module configured for calculating said subject's continuous mean blood pressure values using a Hilbert-Huang transform and an empirical mode decomposition process and based on said received systolic and diastolic blood pressure values and PPG signal.

[0019] According to an exemplary embodiment, the feature extraction module may be further configured generate at least one probabilistic distribution of the calculated distances and provide this information, as a feature information signal, to the blood pressure calculation module.

[0020] According to an exemplary embodiment, the regression module is trained using mathematical models that, from examples of PPG signals, anthropometric characteristics and systolic and diastolic blood pressure from a plurality of subjects, learn the association between the feature vectors computed in the feature extraction module and the corresponding systolic and diastolic blood pressure values.

[0021] According to an exemplary embodiment, the empirical mode decomposition module uses the subject's systolic and diastolic blood pressure values provided by the regression module for shifting the continuous mean blood pressure values to the correct levels of blood pressure.

[0022] According to an exemplary embodiment, the feature extraction module is further configured for receiving a subject's electrocardiogram (ECG) signal, detect a plurality of signal characteristic points on said received ECG signal, calculate a plurality of possible pair-wise distances in both time and amplitude between said detected electrocardiogram signal characteristic points and between said detected ECG signal characteristic points and said PPG signal characteristic

points, and providing a feature information signal comprising information about said calculated distances; and the regression module is further configured for using mathematical models that express the relation between the summarized characteristic point distances of said ECG signal, said PPG signal and a combination of both ECG and PPG, the anthropometric characteristics and the arterial blood pressure levels of the subject.

[0023] According to an exemplary embodiment, the regression module is trained using a linear and/or multiple linear regression model, a random forest regression model, a Bayesian model and/or general machine learning regression model.

[0024] According to an exemplary embodiment, there is provided a method for estimating a subject's blood pressure comprising: receiving a subject's PPG signal and anthropometric characteristics; detecting a plurality of signal characteristic points on said received PPG signal; calculating a plurality of possible pair-wise distances in both time and amplitude between said detected PPG signal characteristic points, calculating said subject's systolic and diastolic blood pressure values using a machine-learning regression model and based on said calculated distances and said anthropometric characteristics; and calculating said subject's continuous mean blood pressure values using a Hilbert-Huang transform and an empirical mode decomposition process and based on said received systolic and diastolic blood pressure values and PPG signal.

[0025] According to an exemplary embodiment, the method for estimating a subject's blood pressure further comprises: receiving the subject's ECG signal; detecting a plurality of signal characteristic points on said received ECG signal; calculating a plurality of possible pair-wise distances in both time and amplitude between said detected ECG signal characteristic points and between said detected ECG signal characteristic points and said PPG signal characteristic points.

Brief description of the drawings

[0026] The above and other aspects of the system and method according to the present description will be shown and explained with reference to the non-restrictive example embodiments described hereinafter.

Figure 1 shows a first general block diagram of an exemplary system for blood pressure estimation according to the present invention.

Figure 2 shows a first block diagram of a feature extraction module according to an exemplary embodiment.

Figure 3 shows a PPG signal window in which a plurality of characteristic points are detected according to an exemplary embodiment.

Figure 4 shows an exemplary block diagram of a blood pressure calculation module according to an embodiment of the present invention.

Figure 5 shows a second general block diagram of an exemplary system for blood pressure estimation according to the present invention.

Figure 6 shows a second block diagram of a feature extraction module according to an exemplary embodiment.

Figure 7 shows an ECG signal window in which a plurality of characteristic points are detected according to an exemplary embodiment.

Figure 8 shows an exemplary graph of the absolute mean error for diastolic and systolic blood pressure values calculated according to an exemplary embodiment of the invention and in comparison to values measured by a blood pressure estimation reference device.

Figure 9 shows an exemplary graph of estimated continuous mean blood pressure signal values calculated according to an exemplary embodiment of the invention and in comparison to signal values measured by a blood pressure estimation reference device.

Detailed description

[0027] In the following, in the description of exemplary embodiments, various features may be grouped together in a single embodiment, figure, or description thereof for the purpose of streamlining the disclosure and aiding in the understanding of one or more of the various inventive aspects. This is however not to be interpreted as the invention requiring more features than the ones expressly recited in the main claim. Furthermore, combinations of features of different embodiments are meant to be within the scope of the invention, as would be clearly understood by those skilled in the art. Additionally, in other instances, well-known methods, structures and techniques have not been shown in detail in order not to obscure the conciseness of the description.

[0028] **Figure 1** shows a first general block diagram of an exemplary electronic system **100** for arterial blood pressure estimation, comprising a feature extraction module **10** and a blood pressure calculation module **20**. The feature extraction module **10** receives a PPG signal **PPG1** and generates a feature information signal **FE**. The blood pressure calculation module **20** receives the PPG signal **PPG1**, the feature information signal **FE** and an anthropometric characteristics

information signal **AC** and generates a systolic blood pressure information signal **SBP**, a diastolic blood pressure information signal **DBP** and a continuous mean blood pressure information signal **CMBP**.

[0029] According to an exemplary embodiment, the anthropometric characteristics information signal **AC** is a signal comprising information about the subject's age, weight and/or height. This information may be input by a subject, received from another electronic device or module and/or already stored in the system.

[0030] According to an exemplary embodiment, the blood pressure calculation module **20** is configured to calculate a systolic, diastolic and/or a mean continuous arterial blood pressure of a living being subject based on a PPG signal **PPG1**, a feature information signal **FE** comprising statistics of the distribution of characteristic points of the PPG signal **PPG1** and anthropometric characteristics **AC** of that subject.

[0031] Figure 2 shows a first exemplary block diagram of a feature extraction module **10** according to an embodiment of the present invention. The feature extraction module **10** comprises a PPG point detection module **11** and a distance computation module **13**. According to an exemplary embodiment, the PPG point detection module **11** receives as input the PPG signal **PPG1**, which may be, for example, the output from a pulseoximeter sensor and which may be received over a hardwired or wireless connection. The PPG signal **PPG1** may also be filtered before being received by the feature extraction module **10**. According to an exemplary embodiment, a certain time window or segment, e.g. 5 seconds, of the received PPG signal or data is collected and temporarily stored in the module, and then the PPG point detection module **11** performs, on that stored PPG signal, a detection of a plurality of PPG signal characteristic points, such as and not limited to, a foot **F1**, an upstroke **U1**, a primary peak **PP1**, a diastolic notch **DN1** and/or a secondary peak **SP1**, as shown in Figure 3. According to an exemplary embodiment, the PPG point detection module **11** may compute characteristic points on the first and second derivative of the PPG signal.

[0032] According to an exemplary embodiment, the detected PPG characteristic points are then provided to the distance computation module **13** in the form of, for example two-dimensional vectors, in which for example, the first coordinate represents the timestamp and the second coordinate the amplitude of the detected points. The distance computation module **13** then calculates a plurality of or all the possible pair-wise distances (in both time and in amplitude) between some or all the coordinates of the received two-dimensional vectors, that is, the distance or difference in time and/or amplitude between any two detected characteristic points. According to an exemplary embodiment, the distance computation module **13** may calculate distances between normalized amplitudes of the PPG signal. The calculated distances are then provided, as a feature information signal **FE**, to the blood pressure calculation module **20**. According to an exemplary embodiment, the distance computation module **13** may further determine statistics of the distribution of such PPG characteristic points and distances and provide at least one probabilistic distribution of the computed distances, such as, but not limited to, one or more histograms, as a feature information signal **FE** to the blood pressure calculation module **20**. According to an embodiment, based on the same distribution, it is possible to compute several histograms based on the width of bins. Those distributions may be aggregated in a final feature vector representing the input to the blood pressure calculation module **20**.

[0033] Figure 4 shows an exemplary block diagram of a blood pressure calculation module **20** according to an embodiment of the present invention. The blood pressure calculation module **20** comprises a first estimation module **21** and a second estimation module **25**. According to an exemplary embodiment, the first estimation module **21** is a machine-learning based regression module that receives the feature information signal **FE** and the anthropometric characteristics information signal **AC** and calculates an estimation of the subject' systolic blood pressure **SBP** and diastolic blood pressure **DBP**.

[0034] According to an exemplary embodiment, the first estimation module **21** is trained using mathematical models that, from examples of PPG signals, anthropometric characteristics and systolic and diastolic blood pressure, learn the association between the feature vectors computed in the feature extraction module **10** and the corresponding systolic and diastolic blood pressure values. Examples of such mathematical models may be, but are not limited to, linear and/or multiple linear regression models, random forest regression models, Bayesian models and/or general machine learning regression models. According to an exemplary embodiment, the parameters of the regression models may be derived using information about statistics of the distance computed by the feature extraction module **10** and arterial blood pressure reference values from a plurality of subjects. The mathematical models express the relation between the summarized distances between characteristic points of a PPG signal, the anthropometric characteristics and the arterial blood pressure levels of the subject.

[0035] According to an exemplary embodiment the first estimation module **21** is a machine-learning based classification and regression module that receives the feature information signal **FE** and the anthropometric characteristics information signal **AC** and calculates an estimation of the subject' systolic blood pressure **SBP** and diastolic blood pressure **DBP**. The first estimation model **21** may use linear and/or multiple linear classification and regression models, random forest classification and regression models, Bayesian models and/or general machine learning classification and regression models. According to an exemplary embodiment, the parameters of the classification and regression models may be derived using information about statistics of the distance computed by the feature extraction module **10** and arterial blood pressure reference values from a plurality of subjects. It shall be noted that a classification and regression model

is a discretized version of a regression model, which could be advantageous for estimation of the subject's systolic and diastolic blood pressure in some applications.

[0036] According to an exemplary embodiment, the second estimation module **25** receives as input the PPG signal **PPG1**, the systolic blood pressure information signal **SBP** and the diastolic blood pressure information signal **DBP** and calculates an estimation of the subject's continuous mean blood pressure **CMBP**. According to an exemplary embodiment, the second estimation module **25** is based on the Hilbert-Huang transform (HHT) and Empirical Mode Decomposition (EMD), wherein the EMD is used for the estimation of the continuous mean arterial blood pressure **CMBP** from the PPG signal. According to an exemplary embodiment, the second estimation module **25** uses the systolic blood pressure information signal **SBP** and the diastolic blood pressure information signal **DBP** provided by the first estimation module **21** for shifting the output of the EMD process (the continuous mean arterial blood pressure **CMBP** values) to the correct levels of blood pressure. This can be done for example by shifting the calculated continuous mean arterial blood pressure values using a mean arterial pressure baseline. The Mean Arterial Pressure value baseline can be calculated according to the formula:

$$\text{Mean Arterial Pressure} = \text{DBP} + (\text{SBP} - \text{DBP})/3$$

[0037] as described in document "How Vascular Hemodynamics Affects Blood Pressure" by Salvi, P. , Pulse Waves, XII, p.138, 2012.

[0038] As it is known in the art, the HHT provides a method of analysing nonstationary and nonlinear time series data. It uses the EMD method to decompose a signal into so-called intrinsic mode functions. For example, in document "Pulse transit time-based blood pressure estimation using hilbert-huang transform", by Zhang et al., Engineering in Medicine and Biology Society, 31st Annual International Conference of the IEEE EMBS, pp.1785-1788, 3-6 Sept 2009, the authors use HHT and EMD for ECG and PPG conditioning before the computation of the Pulse Transit Time (PTT), i.e. they apply EMD for denoising both ECG and PPG and they use the denoised signals for computing a more accurate PTT.

[0039] Figure 5 shows a second general block diagram of an exemplary electronic system **100** for arterial blood pressure estimation, comprising a feature extraction module **10'** and a blood pressure calculation module **20**. The feature extraction module **10'** receives both a PPG signal **PPG1** and an ECG signal **ECG1** and generates a feature information signal **FE'**. The blood pressure calculation module **20** receives the PPG signal **PPG1**, the feature information signal **FE'** and an anthropometric characteristics information signal **AC** and generates a systolic blood pressure information signal **SBP**, a diastolic blood pressure information signal **DBP** and a continuous mean blood pressure information signal **CMBP**.

[0040] According to an exemplary embodiment, the anthropometric characteristics information signal **AC** is a signal comprising information about the subject's age, weight and/or height. This information may be input by a subject, received from another device or module and/or already stored in the system.

[0041] According to an exemplary embodiment, the blood pressure calculation module **20** is configured to calculate a systolic, diastolic and/or a mean continuous arterial blood pressure of a living being subject based on a PPG signal **PPG1**, a feature information signal **FE'** comprising statistics of the distribution of characteristic points of the PPG signal **PPG1**, an ECG signal **ECG1** and anthropometric characteristics **AC** of that subject.

[0042] Figure 6 shows a second exemplary block diagram of a feature extraction module **10'** according to an embodiment of the present invention. The feature extraction module **10'** comprises a PPG point detection module **11**, an ECG point detection module **12** and a distance computation module **13'**.

[0043] According to an exemplary embodiment, the PPG point detection module **11** receives as input the PPG signal **PPG1**, which may be, for example, the output from a pulseoximeter sensor and may be received over a hardwired or wireless connection. The PPG signal **PPG1** may also be filtered before being received by the feature extraction module **10'**. According to an exemplary embodiment, a certain time window or segment, e.g. 5 seconds, of the received PPG signal or data is collected and temporarily stored in the module, and then the PPG point detection module **11** performs, on that stored PPG signal, a detection of a plurality of PPG signal characteristic points, such as and not limited to, a foot **F1**, an upstroke **U1**, a primary peak **PP1**, a dicrotic notch **DN1** and/or a secondary peak **SP1**, as for example shown in Figure 3. According to an exemplary embodiment, the PPG point detection module **11** may detect characteristic points on the first and second derivative of the PPG signal.

[0044] According to an exemplary embodiment, the ECG point detection module **12** receives as input the ECG signal **ECG1**, which may be, for example, the output from an ECG sensor and may be received over a hardwired or wireless connection. The ECG signal **ECG1** may also be filtered before being received by the feature extraction module **10'**. According to an exemplary embodiment, a certain time window or segment, e.g. 5 seconds, of the received ECG signal or data is collected and temporarily stored in the module, and then the ECG point detection module **12** performs, on that stored ECG signal, a detection of a plurality of ECG signal characteristic points, such as and not limited to, a **P1**, **Q1**, **R1**, **S1** and/or **T1** peaks of the cardiac cycles, as shown in Figure 7. According to an exemplary embodiment, the ECG

point detection module **12** may compute characteristic points on the first and second derivative of the ECG signal.

[0045] According to an exemplary embodiment, the detected PPG and ECG characteristic points are then provided to the distance computation module **13'**, each in the form of, for example, two-dimensional vectors, in which for example, the first coordinate represents the timestamp and the second coordinate the amplitude of the detected points. The distance computation module **13'** then calculates some or all the possible pair-wise distances (in both time and in amplitude) between some or all the coordinates of the received two-dimensional vectors for the PPG and ECG signal individually and between the ECG and PPG signals. According to an exemplary embodiment, the distance computation module **13'** may calculate distances between normalized amplitudes of the PPG and ECG signals. The calculated distances are then provided, as a feature information signal **FE'**, to the blood pressure calculation module **20**. According to an exemplary embodiment, the distance computation module **13'** may provide at least three probabilistic distributions of all the computed distances (at least one for the ECG, one for the PPG and one for the distances between the ECG and PPG coordinates), such as, but not limited to, a histogram, as a feature information signal **FE'** to the blood pressure calculation module **20**. According to an exemplary embodiment, those at least three probabilistic distributions may be also aggregated in a final feature vector representing the input to the blood pressure calculation module **20**.

[0046] It shall be noted then that, according to an exemplary embodiment, the blood pressure calculation module **20** may further take in consideration the additional ECG information in order to improve the calculation of the systolic blood pressure **SBP**, the diastolic blood pressure **DBP** and/or the continuous mean blood pressure **CMBP**. For example, according to an exemplary embodiment, the first estimation module **21** is trained using mathematical models that, from examples of ECG and PPG signals, anthropometric characteristics and systolic and diastolic blood pressure, learn the association between the feature vectors computed in the feature extraction module **10'** and the corresponding systolic and diastolic blood pressure values. The mathematical models of the first estimation module **21** may express the relation between the summarized distances between characteristic points of ECG, PPG and a combination of both (relationship between the ECG characteristic points and the PPG characteristic points), the anthropometric characteristics and the arterial blood pressure levels of the subject, e.g. this module may use mathematical models based on information about ECG value distribution, PPG value distributions, a combination of both and anthropometric characteristics of the subject. Examples of such mathematical models may be, but are not limited to, linear and/or multiple linear regression models, random forest regression models, Bayesian models and/or general machine learning regression models. According to an exemplary embodiment, the parameters of the regression models may be derived using information about statistics of the distance computed by the feature extraction module **10'** and arterial blood pressure reference values from a plurality of subjects. According to an embodiment, the regression model may be a discretized version of a regression model and examples of such used models may comprise linear and/or multiple linear classification and regression models, random forest classification and regression models, Bayesian models and/or general machine learning classification and regression models. The parameters of the classification and regression models may be derived using information about statistics of the distance computed by the feature extraction module **10'** and arterial blood pressure reference values from a plurality of subjects. The second estimation module **25** may use non-stationary and non-linear adaptive time-domain methods. Example of such methods may be the use of a Hilbert-Huang Transform to provide a continuous estimation of the mean arterial blood pressure of the subject. The systolic and diastolic blood pressure estimation values provided by the first estimation module **21** may be used by the second estimation module **25** for shifting the output of the EMD process (the continuous mean arterial blood pressure **CMBP** values) to the correct blood pressure values using a mean arterial pressure baseline value as is known in the art.

[0047] **Figure 8** shows an example of the absolute mean error in diastolic and systolic blood pressure values calculated with a reference Continuous Noninvasive Arterial Pressure (CNAP) device and with a system according to an exemplary embodiment of the invention. The models used in the system according to an exemplary embodiment of the invention were derived from data of 20 subjects. The average absolute error is lower than 7 mmHg and complies with standard testing protocol requirements.

[0048] **Figure 9** shows an exemplary comparison graph illustrating the continuous mean blood pressure signal values provided by a reference CNAP device and the continuous mean blood pressure signal values estimated using a method according to an exemplary embodiment of the invention. The models used in the system according to an exemplary embodiment of the invention were derived from data of 20 subjects. Results obtained show a correlation coefficient of 0.83 for all subjects.

[0049] It shall be noted that the system **100** for blood pressure estimation according to embodiments of the invention may be implemented according to hardware and/or software state of the art techniques, comprising for example a microprocessor, microcontroller or digital signal processor that can understand and execute software program instructions. Some programmable hardware logic and memory means may be specifically designed also for executing the method or parts of it according to exemplary embodiments of the invention. It shall be also understood that although, for simplicity, the exemplary embodiments described herein comprise system operations, calculations and methods applied to and during a certain time window or segment of the received signals, the time windows may vary in length and the system operations, calculations and methods herein described may be applied to a plurality of said time windows

of the received signals; the time window length and the number and selection of signal time windows being a design choice.

Claims

1. An electronic system (100) for estimating a subject's blood pressure, comprising:

a feature extraction module (10) configured for receiving a subject's photoplethysmogram signal (PPG1), detecting a plurality of signal characteristic points (F1 to FN, U1 to UN, PP1 to PPN, DN1 to DNN, SP1 to SPN) on said received photoplethysmogram signal (PPG1), calculating a plurality of distances in both time and amplitude between any two of said detected photoplethysmogram signal characteristic points, and providing a feature information signal (FE) comprising information about said calculated distances; and a blood pressure calculation module (20) configured for receiving said photoplethysmogram signal (PPG1), said feature information signal (FE) and anthropometric characteristics (AC) of the subject, and the blood pressure calculation module (20) comprising

- a first estimation module (21) configured for calculating systolic and diastolic blood pressure values (SBP, DBP) of the subject based on said received feature information signal (FE) and anthropometric characteristics (AC), and

- a second estimation module (25) configured for calculating continuous mean blood pressure values (CMBP) of the subject based on said calculated systolic and diastolic blood pressure values (SBP, DBP) and said photoplethysmogram signal (PPG1);

and wherein the first estimation module (21) uses a machine-learning regression model for calculating said systolic and diastolic blood pressure values (SBP, DBP) and the second estimation module (25) uses a Hilbert-Huang transform and an empirical mode decomposition process for calculating said continuous mean blood pressure values (CMBP).

2. A system (100) for estimating a subject's blood pressure according to claim 1 wherein the feature extraction module (10) is further configured generate at least one probabilistic distribution of the calculated distances and provide this information, as a feature information signal (FE), to the blood pressure calculation module (20).

3. A system (100) for estimating a subject's blood pressure according to any preceding claim wherein the first estimation module (21) is trained using mathematical models that, from examples of photoplethysmogram signals, anthropometric characteristics and systolic and diastolic blood pressure values from a plurality of subjects, learn the association between the feature vectors computed in the feature extraction module (10) and the corresponding systolic and diastolic blood pressure values.

4. A system (100) for estimating a subject's blood pressure according to any preceding claim wherein the feature extraction module (10) is further configured for receiving a subject's electrocardiogram signal (ECG1), detecting a plurality of signal characteristic points (P1 to PN, Q1 to QN, R1 to RN, S1 to SN, J1 to JN, T1 to TN) on said received electrocardiogram signal (ECG1), calculating a plurality of distances in both time and amplitude between any two of said detected electrocardiogram signal characteristic points and between any point of said detected electrocardiogram signal characteristic points and any point of said photoplethysmogram signal characteristic points, and providing a feature information signal (FE) comprising information about said calculated distances; and the first estimation module (21) is further configured for using mathematical models that express the relation between the summarized characteristic point distances of said electrocardiogram signal (ECG1), said photoplethysmogram signal (PPG1) and a combination of both, the anthropometric characteristics (AC) and the arterial blood pressure levels of the subject.

5. A system (100) for estimating a subject's blood pressure according to any preceding claim wherein the first estimation module (21) is trained using a linear and/or multiple linear regression model, a random forest regression model, a Bayesian model and/or general machine learning regression model.

6. A system (100) for estimating a subject's blood pressure according to any preceding claim wherein the machine-learning regression model is a discretized version of a regression model.

7. A system (100) for estimating a subject's blood pressure according to claim 6 wherein the regression module is

trained using a linear and/or multiple linear classification and regression model, a random forest classification and regression model, a Bayesian model and/or general machine learning-based classification and regression model.

5 **8.** Electronic device comprising a system (100) for estimating a subject's blood pressure according to any preceding claim.

9. A method for estimating a subject's blood pressure comprising:

10 receiving a subject's photoplethysmogram signal (PPG1) and anthropometric characteristics (AC);
 detecting a plurality of signal characteristic points (F1 to FN, U1 to UN, PP1 to PPN, DN1 to DNN, SP1 to SPN) on said received photoplethysmogram signal (PPG1);
 calculating a plurality of distances in both time and amplitude between any two of said detected photoplethysmogram signal characteristic points;
 15 calculating, based on said calculated distances and said anthropometric characteristics (AC), said subject's systolic and diastolic blood pressure values (SBP, DBP) using a machine-learning regression model; and
 calculating, based on said received systolic and diastolic blood pressure values (SBP, DBP) and photoplethysmogram signal (PPG1), said subject's continuous mean blood pressure values (CMBP) using a Hilbert-Huang transform and an empirical mode decomposition process.

20 **10.** A method for estimating a subject's blood pressure according to claim 9 further comprising:

receiving a subject's electrocardiogram signal (ECG1);
 detecting a plurality of signal characteristic points (P1 to PN, Q1 to QN, R1 to RN, S1 to SN, J1 to JN, T1 to TN) on said received electrocardiogram signal (ECG1); and
 25 calculating a plurality of distances in both time and amplitude between any two of said detected electrocardiogram signal characteristic points and between any of said detected electrocardiogram signal characteristic points (P1 to PN, Q1 to QN, R1 to RN, S1 to SN, J1 to JN, T1 to TN) and any of said photoplethysmogram signal characteristic points (F1 to FN, U1 to UN, PP1 to PPN, DN1 to DNN, SP1 to SPN).

30 **11.** A computer program product comprising computer program code means adapted to calculate a subject's blood pressure according to the method of claims 9 or 10 when said program is run on a computer.

12. A computer readable storage medium comprising a computer program according to claim 11.

Figure 1

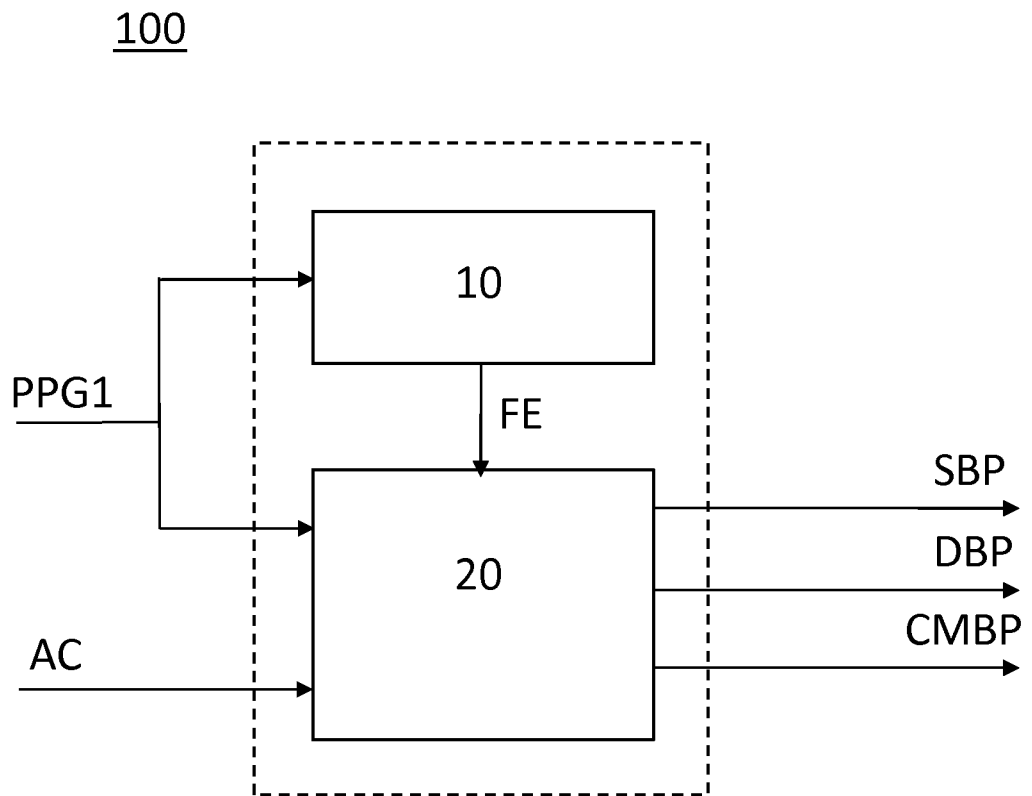


Figure 2

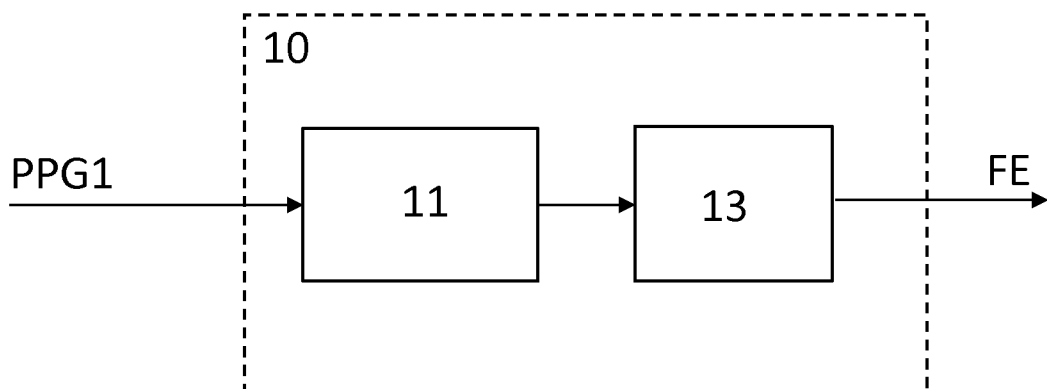


Figure 3

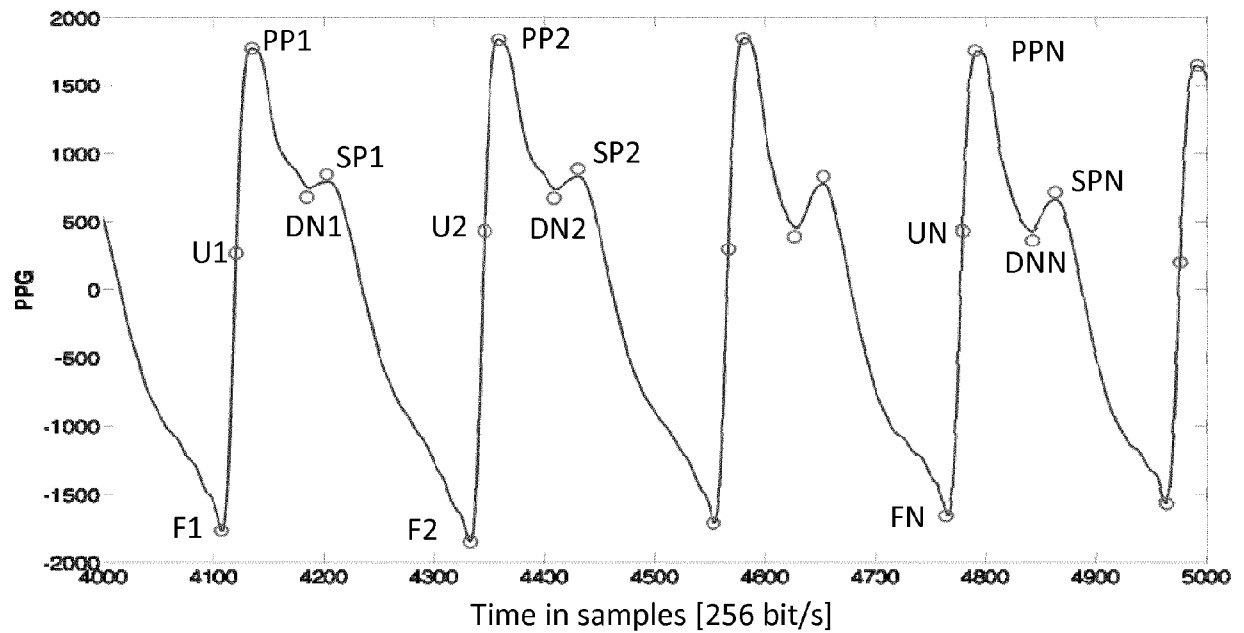


Figure 4

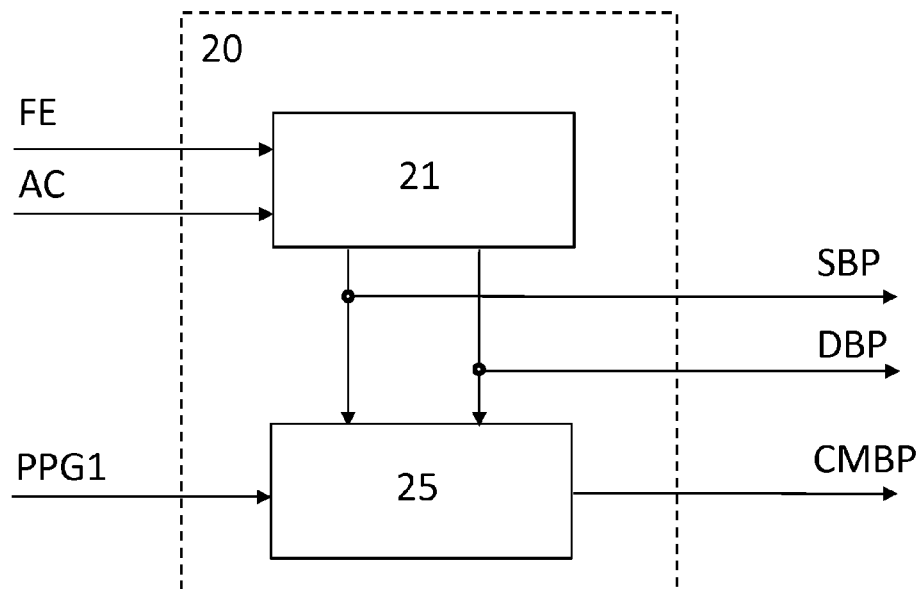


Figure 5

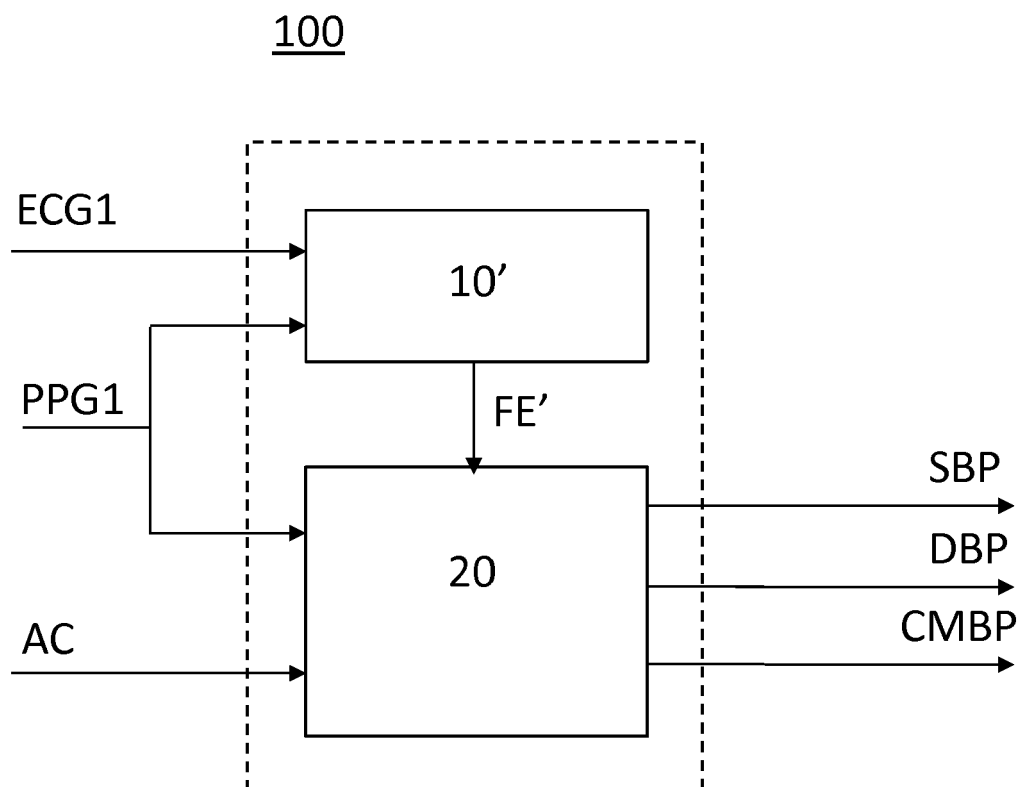


Figure 6

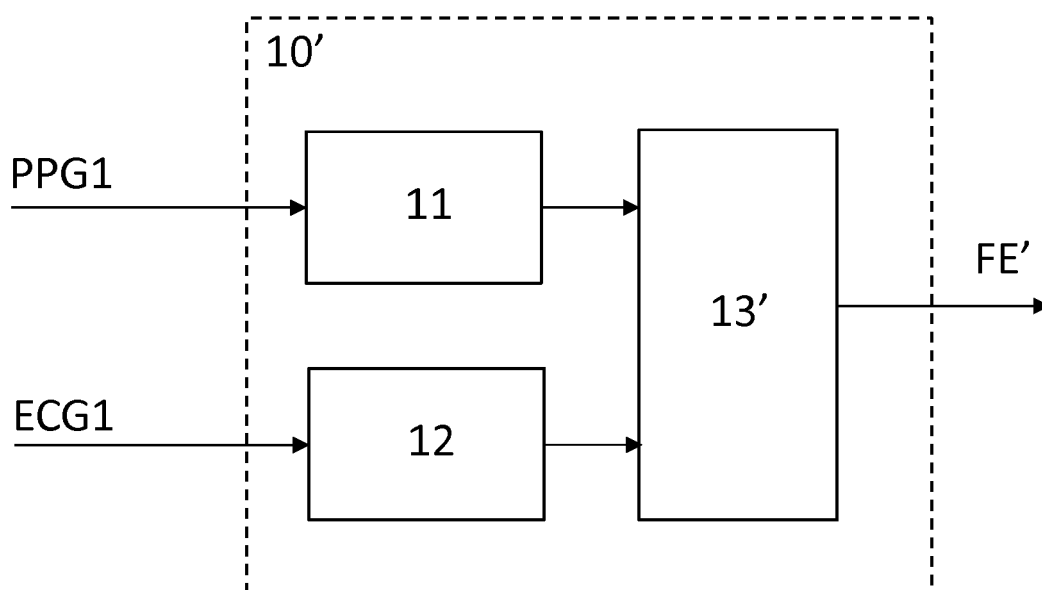


Figure 7

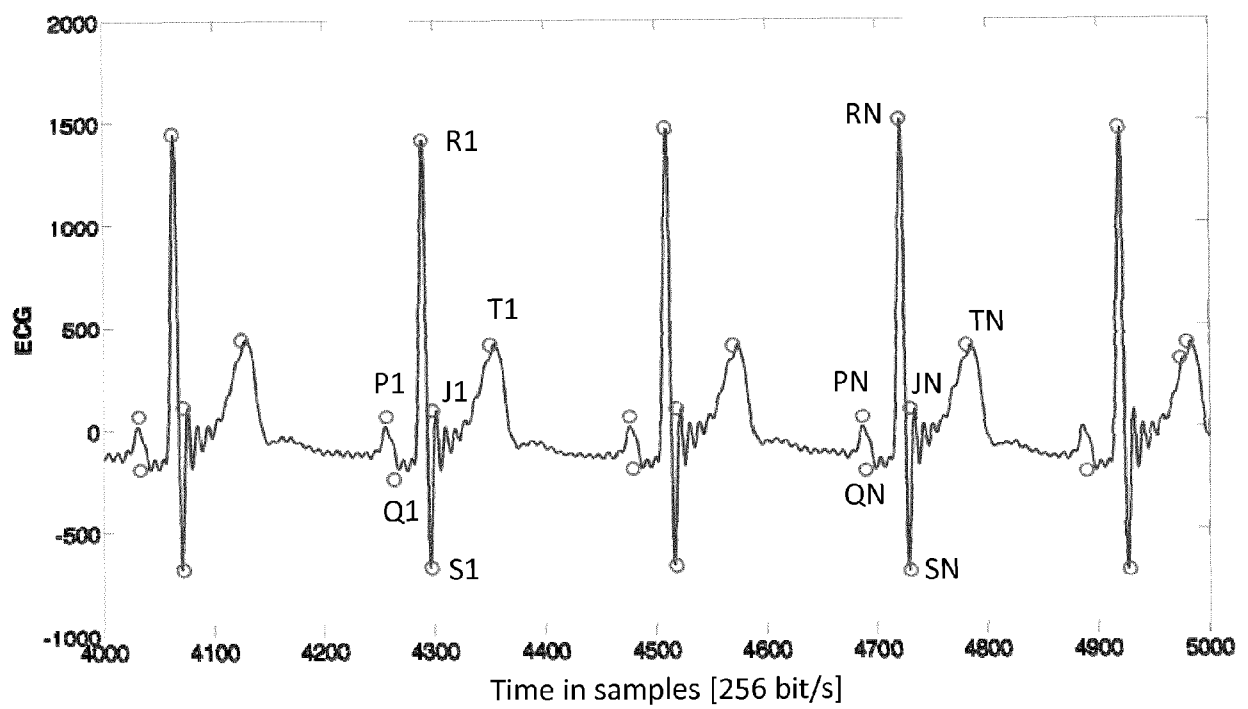


Figure 8

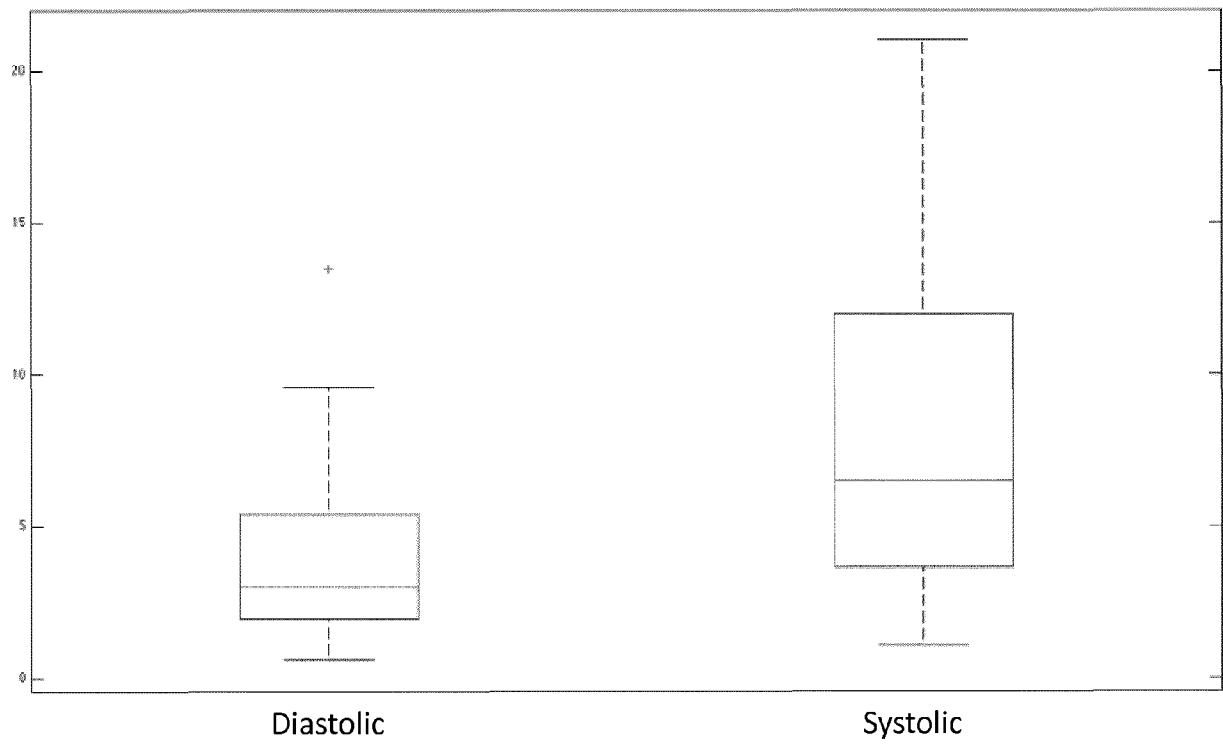
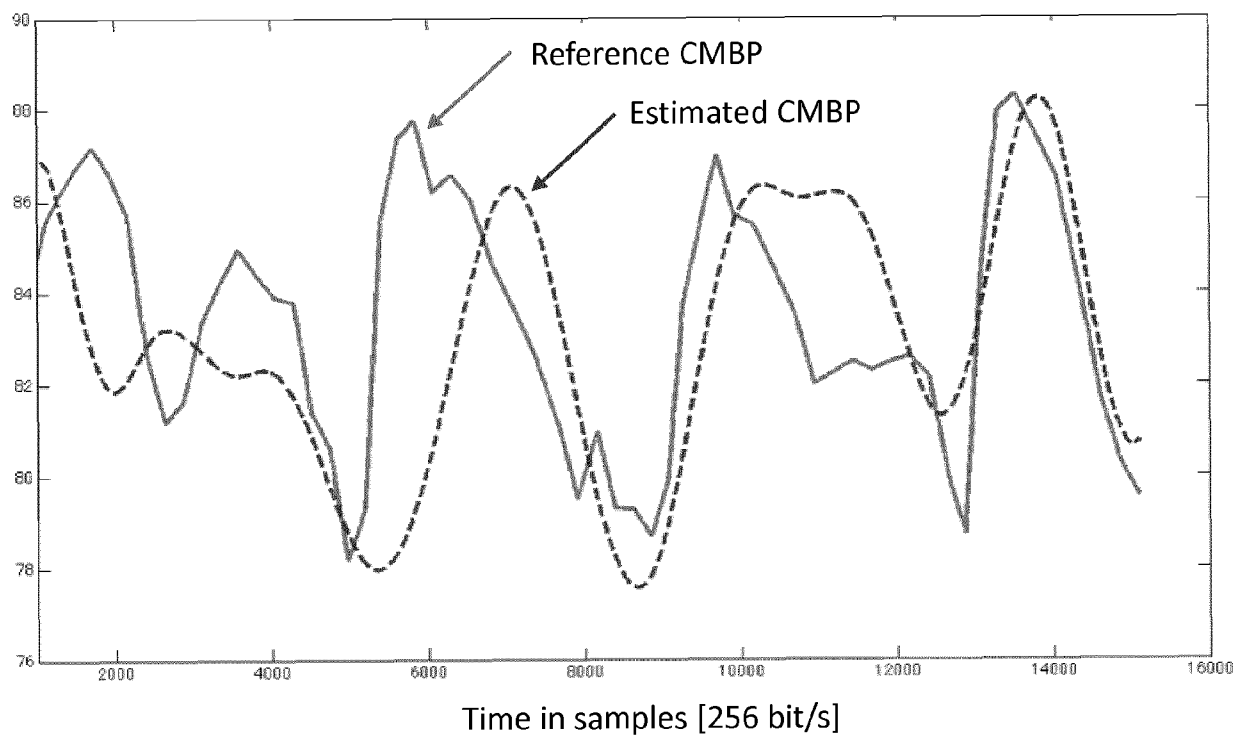


Figure 9





EUROPEAN SEARCH REPORT

Application Number
EP 15 19 8637

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Category	Citation of document with indication, where appropriate, of relevant passages	Relevant to claim	CLASSIFICATION OF THE APPLICATION (IPC)
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A	US 2012/029361 A1 (ADDISON PAUL STANLEY [GB] ET AL) 2 February 2012 (2012-02-02) * paragraph [0050] *	1-12	
A	US 2011/245628 A1 (BAKER JR CLARK R [US] ET AL) 6 October 2011 (2011-10-06) * paragraphs [0023], [0044] *	1-12	
A	US 2014/288446 A1 (LEE CHUN-HO [TW]) 25 September 2014 (2014-09-25) * figure 1 * * paragraph [0027] *	1-12	
A	US 2008/214942 A1 (OH HYUN-HO [KR] ET AL) 4 September 2008 (2008-09-04) * paragraphs [0016] - [0019], [0051] - [0056], [0086] *	1-12	TECHNICAL FIELDS SEARCHED (IPC) A61B
The present search report has been drawn up for all claims			
Place of search The Hague		Date of completion of the search 28 April 2016	Examiner Vanderperren, Yves
CATEGORY OF CITED DOCUMENTS X : particularly relevant if taken alone Y : particularly relevant if combined with another document of the same category A : technological background O : non-written disclosure P : intermediate document T : theory or principle underlying the invention E : earlier patent document, but published on, or after the filing date D : document cited in the application L : document cited for other reasons & : member of the same patent family, corresponding document			

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EPO FORM 1503 03/82 (P04C01)

**ANNEX TO THE EUROPEAN SEARCH REPORT
ON EUROPEAN PATENT APPLICATION NO.**

EP 15 19 8637

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This annex lists the patent family members relating to the patent documents cited in the above-mentioned European search report.
The members are as contained in the European Patent Office EDP file on
The European Patent Office is in no way liable for these particulars which are merely given for the purpose of information.

28-04-2016

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		WO 2012072849 A2	07-06-2012

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EPO FORM P0459

For more details about this annex : see Official Journal of the European Patent Office, No. 12/82

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专利名称(译)	用于血压估计的系统和方法		
公开(公告)号	EP3033991A1	公开(公告)日	2016-06-22
申请号	EP2015198637	申请日	2015-12-09
[标]申请(专利权)人(译)	非盈利IMEC荷兰		
申请(专利权)人(译)	IMEC STICHTING NEDERLAND		
当前申请(专利权)人(译)	IMEC STICHTING NEDERLAND		
[标]发明人	CASALE PIERLUIGI		
发明人	CASALE, PIERLUIGI		
IPC分类号	A61B5/021 A61B5/0295 A61B5/00		
CPC分类号	A61B5/021 A61B5/0295 A61B5/7253 A61B5/7267 A61B5/7278		
审查员(译)	VANDERPERREN , YVES		
优先权	2014197973 2014-12-15 EP		
其他公开文献	EP3033991B1		
外部链接	Espacenet		

摘要(译)

1. 一种用于估计受试者血压的电子系统 (100) , 包括 : 特征提取模块 (10) , 被配置为接收受试者的光电血管容积信号 (PPG1) , 检测所述接收到的光电血管运动信号 (PPG1) 上的多个信号特征点 , 在任何两个所述检测到的光电血管容积信号特征点之间的时间和幅度两者上的多个距离 , 并提供包括关于所述计算的距离的信息的特征信息信号 (FE) 和血压计算模块 (20) , 其被配置为接收所述对象的所述光电血管容积信号 (PPG1) , 所述特征信息信号 (FE) 和人体测量特征 (AC) , 并且所述血压计算模块 (20) 包括第一估计模块 (21) , 其被配置用于基于所述接收到的特征信息信号 (FE) 和人体测量特征 (AC) 来计算所述对象的收缩压和舒张压值 (SBP , DBP) ; 以及第二估计模块 (25) 基于所述计算的收缩压和舒张压值 (SBP , DBP) 和所述光电血管容积图信号 (PPG1) 计算所述对象的连续平均血压值 (CMBP) ; 并且其中所述第一估计模块 (21) 使用机器学习回归模型来计算所述收缩压和舒张压值 (SBP , DBP) , 并且所述第二估计模块 (25) 使用希尔伯特 - 黄变换和经验模式分解过程用于计算所述连续平均血压值 (CMBP) 。

Figure 1

